Consistent inter-protocol differences in resting-state functional connectomes between normal aging and mild cognitive impairment

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Abstract

Resting-state functional connectivity is a promising biomarker for Alzheimer's disease. However, previous resting-state functional magnetic resonance imaging studies in Alzheimer's disease and mild cognitive impairment (MCI) have shown limited reproducibility as they have had small sample sizes and substantial variation in study protocol. We sought to identify functional brain networks and connections that could consistently discriminate normal aging from MCI despite variations in scanner manufacturer, imaging protocol, and diagnostic procedure. We therefore pooled four independent datasets, including 112 healthy controls and 143 patients with MCI, systematically testing multiple brain connections for consistent differences. The largest effects associated with MCI involved the ventromedial and dorsomedial prefrontal cortex, striatum, and middle temporal lobe. Compared with controls, patients with MCI exhibited significantly decreased connectivity within the frontal lobe, between frontal and temporal areas, and between regions of the cortico-striatal-thalamic loop. Despite the heterogeneity of methods among the four datasets, we identified robust MCI-related connectivity changes that appear to be promising candidate biomarkers for Alzheimer's disease.

Keywords: fMRI, mild cognitive impairment, connectome, resting-state, default mode network

1. Introduction

Resting-state connectivity in functional magnetic resonance imaging (fMRI) captures the spatial coherence of spontaneous fluctuations in blood oxygenation. Resting-state fMRI is a promising technique that may be useful as an early biomarker for Alzheimer's disease (AD), a neurodegenerative process that develops over decades before patients suffer from dementia. The possibility that disturbed resting-state connectivity may be an early marker for AD is supported by studies of mild cognitive impairment (MCI), a disorder characterized by objective cognitive deficits without dementia, i.e., without impairment in activities of daily living. These studies showed altered functional connectivity in MCI compared with cognitively normal elderly (NI) (Bai et al., 2009; Liang et al., 2012; Sorg et al., 2007; Wu et al., 2014), but they relied on small sample sizes (n~40) and differed in many aspects of their protocols, e.g. recruitment and image acquisition procedures. If resting-state fMRI is to serve as a useful biomarker of AD for clinical practice or research, changes in functional connectivity must be robust to such variation in study protocols. Therefore, we sought to identify brain connections that showed consistent MCI-related changes across multiple independent studies.

Resting-state connectivity studies have consistently found decreased connectivity between nodes of the default mode network (DMN) in patients with AD or MCI compared with NI (Bai et al., 2009; Koch et al., 2012; Liang et al., 2012; Sorg et al., 2007; Zhang et al., 2010). Less consistent are reports of alterations in the executive attentional, frontoparietal, and anterior temporal networks (Agosta et al., 2012; Gour et al., 2011; Liang et al., 2012; Sorg et al., 2007; Wu et al., 2014; Zhang et al., 2010) due to the literature's bias towards investigating the DMN. Even worse, some studies have reported increased connectivity between the middle temporal lobe and other DMN areas in MCI (Qi et al., 2010), while others have reported decreased connectivity between these same regions (Bai et al., 2009) and others have reported no significant differences between MCI and NI (Koch et al., 2012).

One obvious explanation for such inconsistency may be these studies' small sample sizes resulting in low statistical power (Kelly et al., 2012). Beyond this, however, there are other methodological differences that may compromise the comparison of results across independent studies. For example, the criteria for recruiting subjects with MCI, e.g. Petersen (2004), vs. NIA-AA recommendations (Albert et al., 2011) may differ among studies. Different study samples may also reflect different socio-cultural characteristics of recruiting sites, e.g., ethnicity, language, diet, socioeconomic status. The fMRI measurements themselves can also be affected by differences in details of the image acquisition such as scanner make and model (Friedman et al., 2006), sequence parameters such as repetition time, flip angle, or acquisition volume (Friedman and Glover, 2006), experimental design such as eyes-open/eyes-closed (Yan et al., 2009) or experiment duration (Van Dijk et al., 2010), and scanning environment such as sound attenuation measures (Elliott et al., 1999), room temperature (Vanhoutte et al., 2006), or head-motion restraint techniques (Edward et al., 2000).

To identify robust changes in resting-state connectivity between MCI and NI, we implemented a pooled analysis of four independent resting-state fMRI datasets (ADNI2 and three small single-site studies) using a weighted average implemented by Willer et al (2010) for meta-analysis. Rather than relying on a priori target regions or connections, we leveraged the large sample size to perform a systematic search of brain connections affected by MCI, an approach termed a "connectome-wide association study" (Shehzad et al., 2014). In addition, we relied on functionally-defined brain parcellations using an automated clustering procedure and we explored the impact of the number of brain clusters (called resolution) on observed differences (Bellec et al., 2014).

2. Methods

2.1 Participants

We pooled data from four independent studies: the Alzheimer's Disease Neuroimaging Initiative 2 (ADNI2) sample, two samples from the Centre de recherche de l'institut universitaire de gériatrie de Montréal (CRIUGMa and CRIUGMb), and a sample from the Montreal Neurological Institute (MNI) (Wu et al., 2014). All participants gave their written informed consent to engage in these studies, which were approved by the research ethics board of the respective institutions, and included consent for data sharing with collaborators as well as secondary analysis. Ethical approval was also obtained at the site of secondary analysis (CRIUGM).

The ADNI2 data used in the preparation of this article were obtained from the Alzheimer's Disease Neuroimaging Initiative (ADNI) database (adni.loni.usc.edu). ADNI was launched in 2003 by the National Institute on Aging, the National Institute of Biomedical Imaging and Bioengineering, the Food and Drug Administration, private pharmaceutical companies and non-profit organizations, as a $60 million, 5-year public-private partnership representing efforts of co-investigators from numerous academic institutions and private corporations. ADNI was followed by ADNI-GO and ADNI-2 that included newer techniques. Subjects included in this study were recruited by ADNI-2 from 13 sites across North America. For up-to-date information, see www.adni-info.org.

The combined sample included 112 NI and 143 MCI. In the NI group, the mean age was 72.0 (s.d. 7.0) years, and 38.4% were men. Mean age of the MCI subjects was 72.7 (s.d. 7.7) years, and 50.3% were men. An independent samples t-test did not reveal any significant difference in age between the groups (t = 0.759, p = 0.448). A chi-squared test revealed a trend towards a significant difference in gender distribution between the groups (χ^2 = 3.627, p = 0.057). Note that both age and gender were entered as confounding variables in the statistical analysis below. See Table 1 for sample size and demographic information from the individual studies.

Table 1. Demographic information in all studies

		ADNI2	**CRIUGMa**	**CRIUGMb**	**MNI**	**Combined sample**
NI	N	59	20	18	15	112
	Mean age (s.d.)	74.1 (6.8)	71.7 (8.2)	69.9 (4.9)	67.0 (5.7)	72.0 (7.0)
	Number male	27	7	2	7	43
MCI	N	93	9	22	19	143
	Mean age (s.d.)	71.7 (7.8)	80.7 (6.2)	74.9 (6.9)	71.6 (8.1)	72.7 (7.7)
	Number male	47	4	13	8	72

All subjects underwent cognitive testing (e.g. memory, language, and executive function) (see Supplementary Table 1 for a list of specific tests used in each study). Exclusion criteria common to all studies included: Contraindications to MRI, presence or history of axis I psychiatric disorders (e.g. depression, bipolar disorder, schizophrenia), presence or history of neurologic disease with potential impact on cognition (e.g. Parkinson's disease), and presence or history of substance abuse. NI subjects could not meet criteria for MCI or dementia. Those with MCI had memory complaints, objective cognitive loss (based on neuropsychological testing), but had intact functional abilities and did not meet criteria for dementia. In ADNI2, the diagnosis of MCI was made based on an education adjusted abnormal score on the Logical Memory II subscale (Delayed Paragraph Recall, Paragraph A

only) from the Wechsler Memory Scale and a Clinical Dementia Rating (CDR) of 0.5. In both CRIUGMa and CRIUGMb, the diagnosis of MCI was made based on scores equal to or greater than 1.5 standard deviations below the mean adjusted for age and education on memory tests. At the MNI, the diagnosis of MCI relied on the Petersen criteria (2004). At both CRIUGMb and MNI, MCI diagnoses were made with input from a neurologist. See the Supplementary Methods for greater details for each study.

2.2 Imaging data acquisition

All resting-state fMRI and structural scans were acquired on 3T scanners. We performed analyses on the first usable scan (typically the baseline scan) from ADNI2 and applied clinical diagnoses from that scan for each participant in that dataset. See Table 2 for acquisition parameters for each sample.

Table 2. Structural and functional scan acquisition parameters

		ADNI2[1]	**CRIUGMa**	**CRIUGMb**	**MNI**
	Scanner manufacturer	Philips	Siemens	Siemens	Siemens
Structural	No. channels	8	32	32	32
	No. slices	170	176	176	176
	Slice thickness (mm)	1.2	1	1	1
	In-plane resolution (mm x mm)	1 x 1	1 x 1	1 x 1	1 x 1
	Matrix size	256 x 240	240 x 265	256 x 256	265 x 248
	TR (s)	6.8	2.3	2.53	2.3
	TE (ms)	3.09	2.91	1.64	2.98
	FA (º)	9	9	7	9
Functional	No. runs	1	1	3	3
	No. channels	8	32	32	32
	No. volumes	140	240	150	160
	No. slices	48	33	42	38
	Slice thickness (mm)	3.3	4	3.4	3.6
	In-plane resolution (mm x mm)	3.3 x 3.3	3 x 3	3.4 x 3.4	3.6 x 3.6
	Matrix size	64 x 59	64 x 64	64 x 64	64 x 64
	TR (s)	3	2	2.6	2
	TE (ms)	30	30	30	30
	FA (º)	80	90	90	90

[1]http://adni.loni.usc.edu/wp-content/uploads/2011/04/ADNI_3T_Philips_2.6.pdf

2.3 Computational environment

All experiments were performed using the NeuroImaging Analysis Kit (NIAK[1]) (Bellec et al., 2011) version 0.12.18, under CentOS version 6.3 with Octave[2] version 3.8.1 and the Minc toolkit[3]

[1] http://simexp.github.io/niak/
[2] http://gnu.octave.org

version 0.3.18. Analyses were executed in parallel on the "Guillimin" supercomputer[4], using the pipeline system for Octave and Matlab (Bellec et al., 2012), version 1.0.2. The scripts used for processing can be found on Github[5].

2.4 Pre-processing

Each fMRI dataset was corrected for slice timing; a rigid-body motion was then estimated for each time frame, both within and between runs, as well as between one fMRI run and the T1 scan for each subject (Collins and Evans, 1997). The T1 scan was itself non-linearly co-registered to the Montreal Neurological Institute (MNI) ICBM152 stereotaxic symmetric template (Fonov et al., 2011), using the CIVET pipeline (Ad-Dab'bagh et al., 2006). The rigid-body, fMRI-to-T1 and T1-to-stereotaxic transformations were all combined to resample the fMRI in MNI space at a 3 mm isotropic resolution. To minimize artifacts due to excessive motion, all time frames showing a displacement greater than 0.5 mm were removed (Power et al., 2012). A minimum of 50 unscrubbed volumes per run was required for further analysis (13 NI and 14 MCI were rejected). The following nuisance covariates were regressed out from fMRI time series: slow time drifts (basis of discrete cosines with a 0.01 Hz high-pass cut-off), average signals in conservative masks of the white matter and the lateral ventricles as well as the first principal components (accounting for 95% variance) of the six rigid-body motion parameters and their squares (Giove et al., 2009; Lund et al., 2006). The fMRI volumes were finally spatially smoothed with a 6 mm isotropic Gaussian blurring kernel. A more detailed description of the pipeline can be found on the NIAK website[6] and Github[7].

2.5 Bootstrap Analysis of Stable Clusters (BASC)

We applied a BASC to identify clusters that consistently exhibited similar spontaneous BOLD fluctuations in individual subjects, and were spatially stable across subjects. We first applied a region-growing algorithm to reduce each fMRI dataset into a time x space array, with 957 regions (Bellec et al., 2006). BASC replicates a hierarchical Ward clustering 1000 times and computes the probability that a pair of regions fall in the same cluster, a measure called stability. The region × region stability matrix is fed into a clustering procedure to derive consensus clusters, which are composed of regions with a high average probability of being assigned to the same cluster across all replications. At the individual level, the clustering was applied to the similarity of regional time series, which was replicated using a circular block bootstrap. Consensus clustering was applied to the average individual stability matrix to identify group clusters. The group clustering was replicated via bootstrapping of subjects in the group. A consensus clustering was finally applied on the group stability matrix to generate group consensus clusters.

The cluster procedure was carried out at a specific number of clusters (called resolution). Using a "multiscale stepwise selection" (MSTEPS) method (Bellec, 2013), we determined a subset of resolutions that provided an accurate summary of the group stability matrices generated over a fine grid of resolutions: 4, 6, 12, 22, 33, 65, 111 and 208.

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[3] http://www.bic.mni.mcgill.ca/ServicesSoftware/ServicesSoftwareMincToolKit
[4] http://www.calculquebec.ca/en/resources/compute-servers/guillimin
[5] https://github.com/SIMEXP/mcinet
[6] http://niak.simexp-lab.org/pipe_preprocessing.html
[7] https://github.com/SIMEXP/mcinet/tree/master/preprocess

2.6 Derivation of functional connectomes

For each resolution *K*, and each pair of distinct clusters, the between-clusters connectivity was measured by the Fisher transform of the Pearson's correlation between the average time series of the clusters. The within-cluster connectivity was the Fisher transform of the average correlation between time series inside the cluster. An individual connectome was thus a *K x K* matrix. See Figure 1a-b for an illustration of a parcellation and associated connectome.

2.7 Statistical testing

To test for differences between MCI and NI at a given resolution, we used a general linear model (GLM) for each connection between two clusters. The GLM included an intercept, the age and sex of participants, and the average frame displacement of the runs involved in the analysis. The contrast of interest (MCI – NI) was represented by a dummy covariate coding the difference in average connectivity between the two groups. All covariates except the intercept were corrected to a zero mean (Figure 1c). We estimated the effects independently at each site and pooled them through inverse variance based weighted averaging (Willer et al., 2010) (Figure 1d).

Resolutions below 50 have been suggested to have higher sensitivity based on prior independent work (Bellec et al., 2014). The GLM was first applied at an a priori resolution of $K = 33$, which was the lowest number of clusters for which the default mode network could be clearly decomposed into subnetworks (Supplementary Figure S1). The false-discovery rate (FDR) across connections was controlled at $q^{FDR} \leq 0.1$ (Benjamini and Hochberg, 1995). In addition to the analysis at resolution 33, we assessed the impact of that parameter by replicating the GLM analysis at the 7 resolutions selected by MSTEPS (Supplementary Figure S2). We implemented an omnibus test ($\alpha \leq 0.05$) to assess the overall presence of significant differences between groups, pooling FDR results across all resolutions (Bellec et al., 2014).

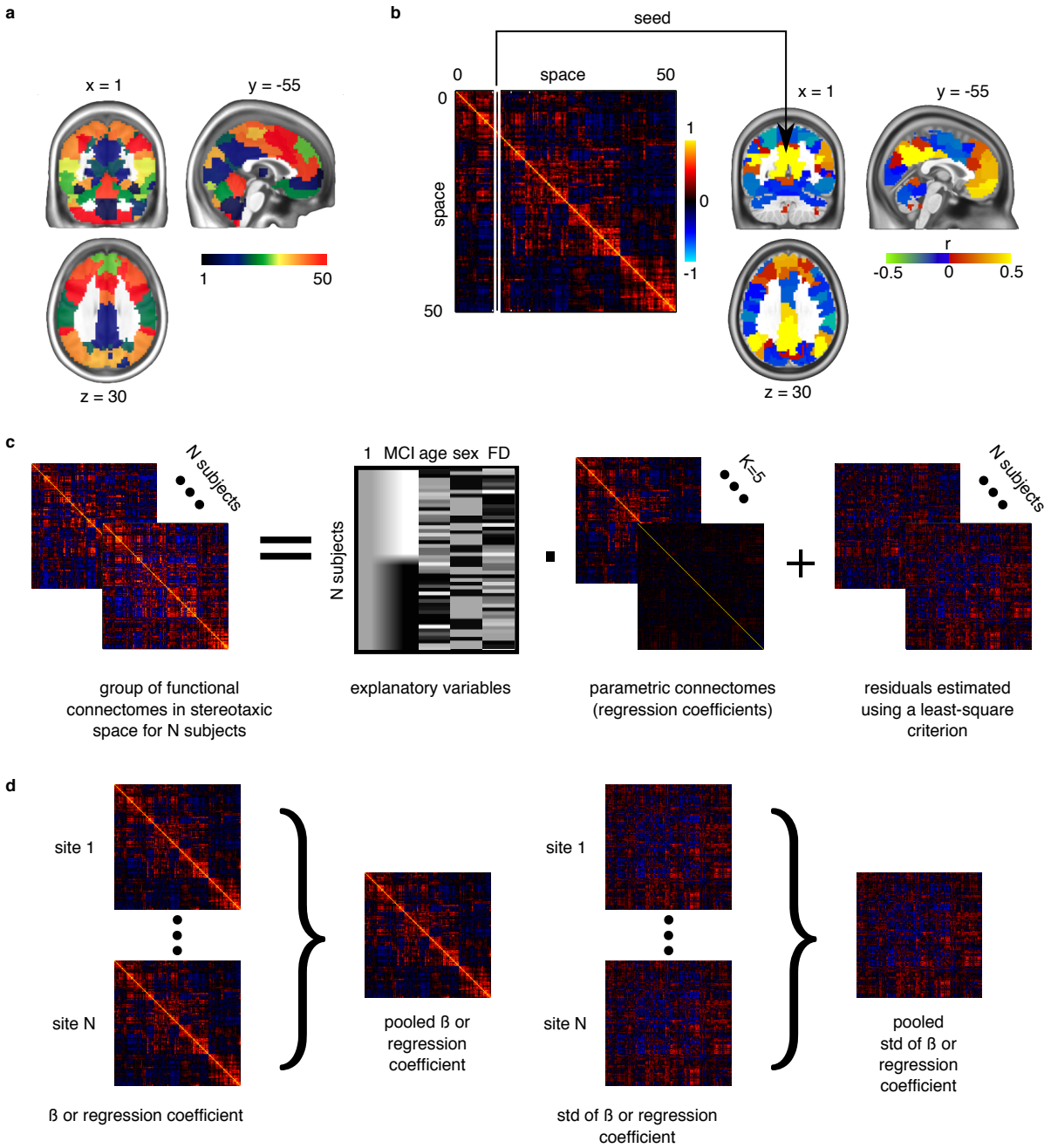

Figure 1. Application of general linear models to connectomes. a) The brain is functionally parcellated into *K* (e.g. 50) clusters generated through a clustering algorithm. b) The connectome is a *K* x *K* matrix measuring functional connectivity between and within clusters. c) A general linear model is used to test the association between phenotypes and connectomes, independently at each connection, at the group level. d) In a multisite situation, independent site-specific effects are estimated and then pooled through weighted averaging (Willer et al., 2010).

3. Results

3.1 Functional connectivity differences between MCI and NI

The omnibus test pooling significant differences in connectivity between MCI and NI across all resolutions was significant at $\alpha \leq 0.05$ ($p = 0.013$). In line with prior observations on independent datasets (Bellec et al., 2014), resolutions below 50 were associated with a higher rate of discovery (Figure 2). At resolution 33, significant group differences between MCI and NI were seen across the whole brain, save for the occipital lobe and cerebellum (Figure 3a). Four brain clusters were associated with 64% of all significant changes found across the connectome: the ventromedial prefrontal cortex, striatum, dorsomedial prefrontal cortex, and middle temporal lobe (Figures 3b, 3c, Supplementary Table 2). Seed-based connectivity using these clusters revealed that MCI showed decreased connectivity between dorsal and ventral frontal areas, between frontal and temporal regions, and between areas of the cortico-striatal-thalamic loop (Figure 4). More specifically, in MCI compared to NI, the ventromedial prefrontal cortex displayed significantly reduced connectivity with dorsal frontal regions and the sensorimotor cortex (Figure 4a). The striatum in MCI exhibited decreased connectivity with the sensorimotor cortex, thalamus, and frontal and parietal regions (Figure 4b). MCI also showed reduced connectivity between the dorsomedial prefrontal cortex with temporal lobe regions, ventral frontal areas, and the cuneus (Figure 4c). Lastly, in MCI, the middle temporal lobe displayed significantly decreased connectivity with the posterior cingulate, precuneus, hippocampus, and frontal areas (Figure 4d).

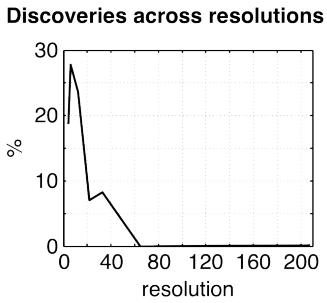

Figure 2. Plot of the percentage of connections identified as significant by the statistical comparison between MCI and NI across the connectome ($q^{FDR} \leq 0.1$), as a function of the resolutions selected by MSTEPS.

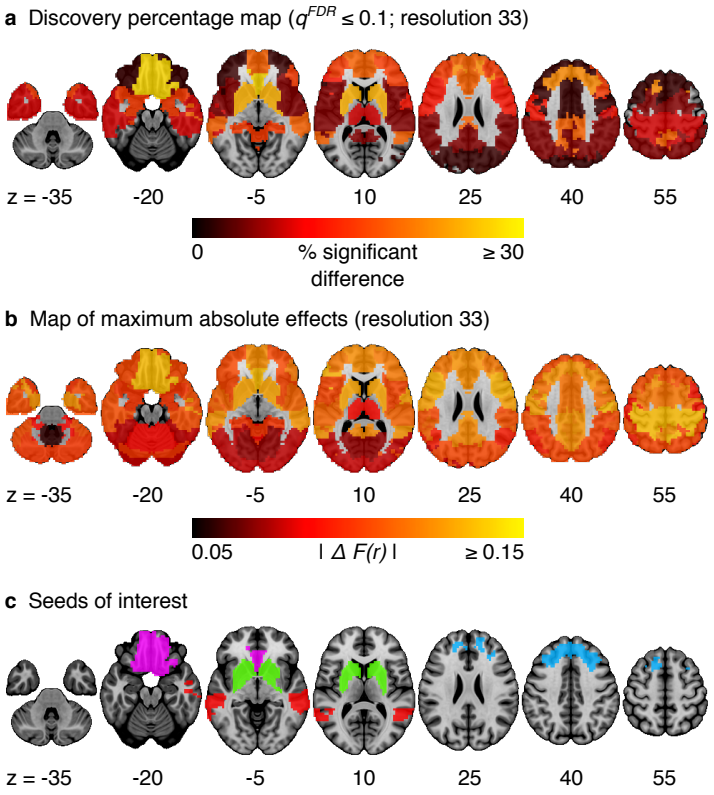

Figure 3. a) Map of the percentage of connections associated with a given cluster and identified as significant by the statistical comparison between MCI and NI, at a resolution of 33 clusters ($q^{FDR} \leq 0.1$). b) Maximum absolute difference in average connectivity between MCI and NI, across all connections associated with a cluster, at resolution 33. c) Four clusters of interest (ventromedial prefrontal cortex, striatum, dorsomedial prefrontal cortex, middle temporal lobe) selected out of 33 for further characterization.

Figure 4. Effect maps for a selection of four seeds that show effects related to MCI at resolution 33. Effect maps reveal the spatial distribution of the changes in functional connectivity for a) the ventromedial prefrontal cortex, b) striatum, c) the dorsomedial prefrontal cortex, and d) the middle temporal lobe. All connections shown in the maps of difference in average connectivity between MCI and NI are significant at $q^{FDR} \leq 0.1$. For each panel, the top line maps the spatial location of the seed region in magenta, the second and third lines show the connectivity (*F(r)*) between the designated seed region and the rest of the brain in NI and MCI respectively, and the fourth line shows a difference map between MCI and NI (*ΔF(r)*).

3.2 Sample-specific effects

The statistical model we used to combine GLM analyses across sites was based on a (weighted) average. The possibility thus existed that an effect would be significant in the pooled analysis because it was driven by a very strong effect in a single sample, instead of being consistent across all samples. By examining effects in each sample independently, we found that MCI-related connectivity changes that surpassed the FDR threshold in the pooled analysis showed similar trends in all samples. For example, the pooled analysis revealed that, compared to NI, MCI exhibited significantly reduced connectivity between the ventromedial prefrontal cortex and dorsal frontal regions, including the sensorimotor cortex. This change appeared to be consistent in all four independent samples (Supplementary Figure S3a). For this particular seed, the change in connectivity was mainly due to regions with positive correlations in NI having smaller correlation values closer to zero in MCI in the individual samples (Supplementary Figure S3b,c).

3.3 Effect of resolution on the GLM

The percentage of discoveries in significant differences between MCI and NI across the connectomes varied markedly as a function of resolution, as selected by the MSTEPS procedure. Higher resolutions were associated with fewer discoveries, especially beyond resolution 65 (Supplementary Figure S4a). By contrast, the maximal amplitude of differences in average connectivity associated with a particular cluster did not decrease substantially, and sometimes increased, when the resolution increased. The decrease in percentage of discovery thus likely reflected a cost associated with an increased number of multiple comparisons in the FDR procedure, rather than a loss in signal quality (Supplementary Figure S4b). Regarding the clusters that were selected for our seed-based analyses (the ventromedial prefrontal cortex, striatum, dorsomedial prefrontal cortex, and middle temporal lobe), the associated effect maps (without statistical threshold) were highly consistent across different resolutions (Supplementary Figures S5-S6), with the potential exception of very low resolutions where, for example, a relatively small cluster like the caudate nuclei got merged with a large distributed cortical network. This also replicated a prior study on the effect of multiresolution parcellations on GLM analysis (Bellec et al., 2014).

4. Discussion

We report resting-state functional connectivity differences in the ventromedial prefrontal cortex, striatum, dorsomedial prefrontal cortex, and middle temporal lobe between MCI and NI subjects that were consistent across multiple studies. Despite protocol differences, we found that MCI exhibited reduced connectivity within the frontal lobe, between frontal and temporal regions, and among areas of the cortico-striatal-thalamic loop compared to NI. Previous studies suggested these altered patterns of functional connectivity in MCI may result from the coevolution of multiple AD-associated biological processes, namely structural degeneration (Coupé et al., 2012; Pievani et al., 2010), neurofibrillary and amyloid pathologies (Small et al., 2006), and cerebrovascular dysfunction (Villeneuve and Jagust, 2015).

The ventromedial prefrontal cortex showed the greatest connectivity changes with other brain areas. Decreased functional connectivity between the ventromedial prefrontal cortex and dorsal regions could reflect degeneration in gray matter and in white matter tracts connecting these areas. Longitudinal studies have shown greater prefrontal cortex atrophy in MCI over time, as well as in those transitioning to AD, compared to NI (Carmichael et al., 2013; McDonald et al., 2009). Cortico-cortical white matter bundles, e.g. superior longitudinal fasciculus, have also been demonstrated to degenerate in patients with MCI and AD (Pievani et al., 2010). Additionally, functional connectivity

changes may reflect the regional effect of increased amyloid burden (Lim et al., 2014; Sheline et al., 2010b), and PIB-PET work has shown the frontal lobe to be one of the first regions in which amyloid accumulates in autosomal dominant AD mutation carriers (Bateman et al., 2012). Our results may also be due to neurofibrillary pathology as it typically appears in the prefrontal cortex during MCI (Bossers et al., 2010). Lastly, cerebral hypoperfusion in the frontal lobe of MCI (Chao et al., 2009) may have contributed to our results.

As expected, a large effect was also observed in the temporal lobe, a region known to suffer from significant AD pathology in preclinical phases (Guillozet et al., 2003). Compared to NI, we found that MCI displayed reduced connectivity between the middle temporal lobe and large parts of the frontal lobe, hippocampus, posterior cingulate and precuneus. This conforms to previous resting-state studies in MCI and AD that have shown effects in the default mode network (Koch et al., 2012; Sorg et al., 2007). Again, we observed functional disconnection between the temporal and frontal lobes in MCI when the dorsomedial prefrontal cortex was selected as a seed. Structural connectivity may explain the functional connectivity changes in these areas, since degeneration of white matter tracts between frontal and temporal regions, e.g. the uncinate fasciculus, occurs with the progression from MCI to AD and correlates with episodic memory impairment in MCI (Pievani et al., 2010; Rémy et al., 2015). Furthermore, examining the integrity of the arcuate fasciculus, a major language tract that connects the frontal and temporal lobes (Dick and Tremblay, 2012), might reveal a biological basis for language impairments such as word-finding difficulties in MCI and AD, (Nutter-Upham et al., 2008). Brain areas that subserve language function could be important targets to investigate given recent evidence that multilingualism may help delay the onset of AD (Chertkow et al., 2010).

Unexpectedly, we also found significant effects in the striatum, which showed reduced connectivity in MCI with sensorimotor cortex, frontal and parietal regions, and thalamus. While not initially expected, these findings may reflect earlier observations that regions within the cortico-striatal-thalamic loops are vulnerable to AD pathology. For example, previous work demonstrated the presence of substantial amyloid burden in the striatum in both autosomal dominant and sporadic forms of AD (H. Braak and E. Braak, 1990; Villemagne et al., 2009), and the striatum may be the first region in which amyloid deposition occurs in autosomal dominant AD (Bateman et al., 2012; Klunk et al., 2007). Furthermore, significant neurodegeneration is known to occur with AD in the striatum and thalamus (de Jong et al., 2008; Madsen et al., 2010), so our results might reflect the brain's capacity for functional plasticity in response to amyloid or neurodegeneration in these regions. Motor cortex hyperexcitability has also been shown in AD, and this suggests that inhibitory circuits leading to the motor cortex may be affected in the disease (Ferreri et al., 2011). Our results may support that theory. Additionally, our findings may represent a biological basis for the cognitive and motor symptoms of MCI (Aggarwal et al., 2006) since the striatum and the rest of the basal ganglia have been implicated in stimulus-response associative learning and memory and motor skill acquisition and execution (Doyon et al., 2009; Packard and Knowlton, 2002). Future research should examine the potential relationship between connectivity in the cortico-striatal-thalamic loops and motor function in MCI and AD.

The consistency of our findings contrasted with previous, smaller single-site studies that have variously reported decreased and increased connectivity. The reports of increased connectivity (Bai et al., 2009; Gour et al., 2011; Qi et al., 2010) may have reflected unique attributes of particular protocols or the choices made with respect to pre-processing steps, for example using global signal regression (Saad et al., 2012).

Among our study's limitations is its cross-sectional nature, which precludes inference that the functional changes we found would necessarily predict progression towards Alzheimer's dementia. Also, we did not account for structural atrophy, despite a bias for increased detection in functional differences due to differences in underlying structure (Dukart and Bertolino, 2014). However MCI-related gray matter changes likely co-localize to some extent with functional changes, and the aim of our work was to map out functional changes rather than study their interaction with atrophy. We did

not account for other variables, such as APOE genotype (Sheline et al., 2010a), amyloid deposition (Sheline et al., 2010b), presence of neurofibrillary tangles (Maruyama et al., 2013), and cerebrovascular mechanisms (Villeneuve and Jagust, 2015). At least some of these could potentially have explained the observed MCI-related functional connectivity changes as part of an underlying disease mechanism. Large-scale multimodal studies, incorporating genomics, proteomics, and multimodal imaging will be needed to identify the interactions between these and other physiological facets of the pathology.

Overall, our results supported previous findings of DMN connectivity changes in AD and MCI (Greicius et al., 2004; Sorg et al., 2007), given that three of the identified seeds (ventromedial prefrontal cortex, dorsomedial prefrontal cortex, middle temporal lobe) are part of this network. It is noteworthy, however, that our strongest observed effects reported were not in the same DMN regions typically described in earlier resting-state studies of MCI and AD, viz, posterior cingulate/precuneus (Sheline et al., 2010b; Zhang et al., 2010). Unexpected changes were also found in the striatum, and this may reflect the advantages of "mining" the whole-brain connectome to search for new biomarkers of mild cognitive impairment and possibly the early progression of the pathophysiologic substrate of Alzheimer's disease. If confirmed, our results could suggest the utility of these regions in resting-state fMRI as a biomarker endpoint in clinical trials. Future research should therefore not only attempt to verify our findings, but also to extend them to cohorts that include Alzheimer's dementia and to longitudinal studies that characterize individuals' progression to dementia.

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