Adjudicating between face-coding models with individual-face fMRI responses

Short title: Adjudicating between face-coding models with fMRI

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Abstract

The perceptual representation of individual faces is often explained with reference

to a norm-based face space. In such spaces, individuals are encoded as vectors where

identity is primarily conveyed by direction and distinctiveness by eccentricity. Here we

measured human fMRI responses and psychophysical similarity judgments of individual

face exemplars, which were generated as realistic 3D animations using a computer-

graphics model. We developed and evaluated multiple neurobiologically plausible

computational models, each of which predicts a representational distance matrix and a

regional-mean activation profile for 24 face stimuli. In the fusiform face area, a face-

space coding model with sigmoidal ramp tuning provided a better account of the data

than one based on exemplar tuning. However, an image-processing model with

weighted banks of Gabor filters performed similarly. Accounting for the data required

the inclusion of a measurement-level population averaging mechanism that

approximates how fMRI voxels locally average distinct neuronal tunings. Our study

demonstrates the importance of comparing multiple models and of modeling the

measurement process in computational neuroimaging.

Author Summary

Humans recognize conspecifics by their faces. Understanding how faces are recognized is an open computational problem with relevance to theories of perception, social cognition, and the engineering of computer vision systems. Here we measured brain activity with functional MRI while human participants viewed individual faces. We developed multiple computational models inspired by known response preferences of single neurons in the primate visual cortex. We then compared these neuronal models to patterns of brain activity corresponding to individual faces. The data were consistent with a model where neurons respond to directions in a high-dimensional space of faces. It also proved essential to model how functional MRI voxels locally average the responses of tens of thousands of neurons. The study highlights the challenges in adjudicating between alternative computational theories of visual information processing.

Introduction

Humans are expert at recognizing individual faces, but the mechanisms that support

this ability are poorly understood. Multiple areas in human occipital and temporal

cortex exhibit representations that distinguish individual faces, as indicated by

successful decoding of face identity from functional MRI (fMRI) response patterns (1–

10). Decoding can reveal the presence of face-identity information as well as

invariances. However, the nature of these representations remains obscure because

individual faces differ along many stimulus dimensions, each of which could plausibly

support decoding. To understand the representational space, we need to formulate

models of how individual faces might be encoded and test these models with responses

to sufficiently large sets of face exemplars. Here we use representational similarity

analysis (RSA) (11) to test face-coding models at the level of the representational

distance matrices they predict. Comparing models to data in the common currency of

the distance matrix enables us to pool the evidence over many voxels within a region,

obviating the need to fit models separately to noisy individual fMRI voxels.

Many cognitive and neuroscientific models of face processing do not make

quantitative predictions about the representation of particular faces (12,13). However,

such predictions can be obtained from models based on the notion that faces are

encoded as vectors in a space (14). Most face-space implementations apply principal

components analysis (PCA) to face images or laser scans in order to obtain a space,

where each component is a dimension and the average face for the training sample is

located at the origin (15,16). In such PCA face spaces, eccentricity is associated with

judgments of distinctiveness, while vector direction is associated with perceived

identity (17–19). Initial evidence from macaque single-unit recordings and human fMRI

suggests that brain responses to faces are strongly modulated by face-space eccentricity,

with most studies finding increasing responses with distinctiveness (20–23). However,

there has been no attempt to develop a unified account for how a single underlying face-

space representation can support both sensitivity to face-space direction at the level of

multivariate response patterns and sensitivity to eccentricity at the level of regional-

mean fMRI activations. Here we develop and evaluate several face-space coding models,

which differ with respect to the proposed shape of the neuronal tuning functions across

face space and with respect to the distribution of preferred face-space locations over the

simulated neuronal population.

Face-space coding models define high-level representational spaces, which are

assumed to arise through unspecified low-level featural processing. An alternative

possibility is that some cortical face-space representations can be explained directly by

low-level visual features, which typically covary with position in PCA-derived face

spaces. To explore this possibility, we evaluated a Gabor-filter model, which receives

stimulus images rather than face-space coordinates as input, and has previously been

used to model response preferences of individual voxels in early visual cortex (24).

We found that cortical face responses measured with fMRI strongly reflect face-

space eccentricity: a step along the radial axis in face space results in a much larger

pattern change than an equal step along the tangential axis. These effects were

consistent with either a sigmoidal-ramp-tuning or a Gabor-filter model. The

performance of these winning models depended on the inclusion of a measurement-

level population-averaging mechanism, which accounted for local averaging of neuronal

tunings in fMRI voxel measurements.

Results

Sampling face space with photorealistic but physically-controlled animations

In order to elicit strong percepts of the 3D shape of each individual face, we generated a set of photorealistic animations of face exemplars. Each 2s animation in the main experiment featured a face exemplar in left or right half profile, which rotated outward continuously (S2 Movie, Experimental Procedures). The animations were based on a PCA model of 3D face shape and texture (25). Each frame of each animation was cropped with a feathered aperture and processed to equate low-level image properties across the stimulus set (Experimental Procedures). We generated 12 faces from a slice through face space (Figure 1b). Euclidean distances between the Cartesian coordinates for each face were summarized in a distance matrix (Figure 1a), which served as the reference for comparisons against distances in the perceptual and cortical face spaces (Figure 1c-h). We generated a physically distinct stimulus set with the same underlying similarity structure for each participant by randomizing the orientation of the slice through the high-dimensional PCA space (for examples, see S1 Figure). This served to improve generalizability by ensuring that group-level effects were not strongly influenced by idiosyncrasies of face exemplars drawn from a particular face-space slice. In formal terms, group-level inference therefore treats stimulus as a random effect (26).

Figure 1. Face spaces obtained from a reference PCA model, perceptual similarity judgments and fMRI response patterns in human visual cortex. (**a-b**) We generated 12 faces in a polar grid arrangement on a 2D slice through the reference PCA space (3 eccentricity levels and 4 directions). The grid was centered on the stimulus space norm (not shown). Euclidean distances between the 12 faces are illustrated in a distance matrix (a) and in a 2D visualization of these distances (b, multidimensional scaling, metric-stress criterion). (**c-d**) Group-average perceptual face space (N=10) estimated from psychophysical similarity judgments. The distance matrix depicts the percentage of trials on which each pair of faces was rated as relatively more dissimilar. (**e-h**) Group-average cortical face-space (N=10) estimated from fMRI response patterns in human visual cortex. The distance matrices depict a cross-validated estimate of multivariate discriminability where 0 corresponds to chance-level performance (Experimental Procedures). Each cortical region was defined in individual participants using independent data. The distance matrices use separate color scales since we expect variable effect sizes across cortical regions. For data from other regions of interest, see S2 Figure.

Cortical face spaces are warped relative to the reference PCA space

Human participants (N=10) participated in a perceptual judgment task (S1 Movie,

2145 trials over 4 sessions) followed by fMRI scans (S2 Movie, 2496 trials over 4

recording days). Brain responses were analyzed separately in multiple independently

localized visual regions of interest. We compared representational distance matrices

estimated from these data sources to distances predicted according to different models

using the Pearson correlation coefficient. These distance-matrix similarities were

estimated in single participants and the resulting coefficients were Z-transformed and

entered into a summary-statistic group analysis for random-effects inference

generalizing across participants and stimuli (Experimental Procedures).

We observed a strong group-average correlation between distance matrices

estimated from perceptual dissimilarity judgments and Euclidean distances in the

reference PCA space (mean(r)=0.83, mean(Z(r))=1.20, standard error=0.05, p<0.001,

Figure 1c, Figure 5a, S1 Table). Correlations between the reference PCA space and

cortical face spaces were generally statistically significant, but smaller in magnitude

(Figure 5b-c, S5 Figure, S1 Table). Distances estimated from the fusiform face area were

weakly, but highly significantly correlated with the reference PCA space (mean(r)=0.17,

mean(Z(r))=0.17, standard error=0.04, p<0.001, Figure 5c). Distances estimated from

the early visual cortex were even less, though still significantly, correlated with the

reference PCA space (mean(r)=0.07, mean(Z(r))=0.07, standard error=0.04, p=0.044,

Figure 5b). These smaller correlations in cortical compared to perceptual face spaces

could not be attributed solely to lower functional contrast-to-noise ratios in fMRI data,

because the effects generally did not approach the noise-ceiling estimate for the sample

(shaded region in Figure 5). The noise ceiling was based on the reproducibility of

distance matrices between participants (Experimental Procedures). Instead, these

findings indicate that the reference PCA space could not capture all the explainable

dissimilarity variance in cortical face spaces.

Cortical face spaces over-represent eccentricity

We quantified the apparent warps in the cortical face spaces by constructing a

multiple-regression RSA model, with separate distance-matrix predictors for

eccentricity and direction, and for within and across face viewpoints (Figure 2a,

Experimental Procedures). These predictors were scaled such that differences between

the eccentricity and direction parameters could be interpreted as warping relative to a

veridical encoding of distances in the reference PCA face space. We also observed strong

viewpoint effects in multiple regions, including the early visual cortex (Figure 1e-f).

Such effects were modeled by separate constant terms for distances within and across

viewpoint.

Eccentricity changes had a consistently greater effect on representational patterns

than direction changes, suggesting that a step change along the radial axis resulted in a

larger pattern change than an equivalent step along the tangential axis (Figure 2c-d).

The overrepresentation of eccentricity relative to direction was observed in each

participant, and in both cortical and perceptual face spaces, although the effect was

considerably larger in cortical face spaces. A repeated-measures two-factor ANOVA

(eccentricity versus direction, within versus across viewpoint) on the single-participant

parameter estimates from the multiple-regression RSA model was consistent with these

apparent differences, with a statistically significant main effect of eccentricity versus

direction for perceptual and cortical face spaces (all $p<0.012$, S2 Table). Thus, compared

to the encoding in the reference PCA space, cortical face spaces over-represented the

radial, distinctiveness-related axis compared to the tangential, identity-related axis.

Figure 2. Face-space warping reflects an over-representation of eccentricity over direction information. (**a**) Squared distances in the reference PCA space were parameterized into predictors coding all 4 combinations of face-space metric (direction, eccentricity) and viewpoint (within, across). This multiple regression RSA model also included separate constant terms for each viewpoint, and was fitted separately to each face space using ordinary least squares (Experimental Procedures). Importantly, the scaling of the eccentricity and direction predictors ensures that equal parameter estimates corresponds to a preserved reference PCA space. (**b**) Multiple regression fit to the perceptual face space with group-average parameter estimates, distance matrix, fitted distances and residuals. Gray lines reflect single participant parameter estimates (**c-d**) Multiple regression fit to the cortical face spaces, plotted as in b. See S2 Table for inferential statistics.

Although these findings suggest a larger contribution of face-space eccentricity than

direction in visual cortex, we also observed clear evidence for greater-than-chance

discrimination performance among faces that differed only in face-space direction.

Group-average cross-validated discriminant distances for faces that differed in direction

but not eccentricity exceeded chance-level performance ($p<0.05$) for typical and

caricatured faces in both the early visual cortex and the fusiform face area (S3 Figure).

Sub-caricatured faces were less consistently discriminable. Indeed, direction

discrimination increased with eccentricity both within (mean=0.013, standard

error=0.007, p=0.036) and across (mean=0.012, standard error=0.005, p=0.016)

viewpoint in the fusiform face area (linear effect of sub>typical>caricature), suggesting

that direction discrimination increased with face-space eccentricity in a dose-dependent

manner (S3 Table). By contrast, within viewpoint discrimination performance in the

early visual cortex scaled with eccentricity (mean=0.039, standard error=0.008,

$p<0.001$), but distances that spanned a viewpoint change did not vary with eccentricity

(mean=0.009, standard error=0.019, p=0.297). This is consistent with a view-dependent

representation in early visual cortex. Thus, cortical regions discriminate identity-related

direction information even in the absence of a difference in distinctiveness-related

eccentricity information, suggesting that cortical face representations cannot be

reduced to a one-dimensional code based on distinctiveness alone. In summary, cortical

coding of face-space position is systematically warped relative to the reference PCA

space, with a substantial overrepresentation of eccentricity and a smaller, but reliable

contribution of face-space direction.

Regional-mean fMRI activation increases with face-space eccentricity,

but removing such effects does not substantially alter cortical face-

space warping

Cortical face-space warping could not be explained by regional-mean activation

preferences for caricatures. We performed a regional-mean analysis of responses in

each cortical area, which confirmed previous reports that fMRI responses increase with

distinctiveness across much of visual cortex (Figure 6, S6 Figure) (23). In order to test

the influence of such regional-mean activation effects on representational distances, we

adapted our discriminant distance metric to remove additive and multiplicative overall

activation effects (Experimental Procedures). Distance matrices estimated using this

alternative method were highly similar to ones estimated without removal of overall

activation effects (all r=0.9 or greater for the Pearson correlation between group-

average distance matrices with and without mean removal, S4 Figure). Thus, although

eccentricity affected the overall activation in all visual areas, the warping of the cortical

face spaces could not be attributed to overall activation effects alone.

Accounting for cortical and perceptual face spaces with PCA face-

space-tuning models and image-computable models

We developed multiple computational models, each of which predicts a

representational distance matrix and a regional-mean activation profile. These models

can be divided into three classes: the sigmoidal-ramp tuning and exemplar tuning

models receive face-space coordinates as input, while the Gabor-filter model receives

gray-scale pixel intensities from the stimulus images as input. We evaluated each of

these three model classes with and without a measurement-level population-averaging

mechanism, which approximates how fMRI voxels locally average underlying neural

activity.

The sigmoidal-ramp-tuning model proposes that the representational space is

covered with randomly oriented ramps, each of which exhibits a monotonically

increasing response along its preferred direction in face space (Figure 3a). This model is

inspired by known preferences for extreme feature values in single units recorded from

area V4 and from face-selective patches in the macaque visual cortex (20,27,28). We

modeled the response along each model neuron's preferred direction using a sigmoidal

function with two free parameters, which control the horizontal offset and the

saturation of the response function (Experimental Procedures). A third parameter

controlled the strength of measurement-level population averaging by translating each

individual model unit's response toward the population-mean response. The way this

accounts for local averaging by voxels is illustrated for the fusiform face area in Figure

3a-b. It can be seen that measurement-level population averaging introduces a

substantial U-shape in the individual response functions, with only a minor deflection in

favor of a preferred face-space direction. At the level of Euclidean distances between

population response vectors evoked by each face, this leads to exaggerated distances for

radial relative to tangential face differences (Figure 3c). In summary, measurement-level

population averaging provides a simple means to interpolate between two extreme

cases: A value of 0 corresponds to the case where the model's response is perfectly

preserved in the fMRI voxels, whereas a value of 1 corresponds to the case where the

model's response to a given stimulus is reduced to the arithmetic mean over the model

units.

In the exemplar model, each unit prefers a location in face space, rather than a

direction, and its tuning is described by a Gaussian centered on the preferred location.

The representational space is covered by a population of units whose preferred

locations are sampled from a Gaussian centered on the norm face (Figure 3d,

Experimental Procedures). We fitted the Gaussian exemplar-tuning model similarly to

the sigmoidal ramp-tuning model, using two parameters that controlled the width of the

Gaussian tuning function and the width of the Gaussian distribution from which

preferred faces were sampled. We also evaluated a variant of the exemplar model where

the distribution of preferred faces followed an inverted-Gaussian distribution (Figure

3e). Population averaging was modeled in the same way as for the sigmoidal-ramp-

tuning model using a third parameter.

Figure 3. Computational models for face-space coding based on sigmoidal ramp or exemplar tuning coupled with measurement-level population averaging. The visualization uses the model parameters that were optimal for predicting the face space in the fusiform face area. (**a**) Response function from the sigmoidal ramp model's internal representation (left panel) and its measurement (right panel) following translation toward the population-average response function (middle panel). (**b**) Two-dimensional generalization of the sigmoidal ramp tuning function to encode a direction in the face-space slice. An example unit is plotted in the left and right panels with the population-average response in the middle panel. (**c**) The model's representational dissimilarity structure was estimated as the Euclidean distance between the population response vectors elicited by a coordinate in the face-space slice (white circle) and every other coordinate on the face space slice. Two example coordinates are plotted in the left and right panels. It can be seen that dissimilarity increases more rapidly with radial (eccentricity) than with tangential (direction) face-space distance. (**d**) Two-dimensional response function for an example unit from the Gaussian exemplar model (white marker). A sub-set of other units is overlaid in black markers to illustrate the width of the Gaussian distribution of tuning centers. (**e**) Two-dimensional response function for an example unit from the negative Gaussian exemplar model, plotted as in panel d.

245   The Gabor-filter model differs from the previous model classes in that it receives

246  gray-scale image intensities as input, rather than face-space position (Figure 4a). Such

247  models have previously been used to account for response preferences of individual

248  voxels in early visual cortex (24). The model comprises Gabor filters varying in

249  orientation, spatial frequency and phase, and spatial position. The filters are organized

250  into banks, each corresponding to a spatial frequency and comprising a different

251  number of spatial positions (coarser for lower spatial frequencies; Figure 4b,

252  Experimental Procedures). We assumed that all orientations and spatial positions are

253  equally represented. For the spatial frequencies, however, we let the data determine the

254  weighting. We fitted a weighted representational model with one weight for each

255  spatial-frequency bank (5 free parameters, Figure 4c). Local averaging in fMRI voxels

256  was modeled using two stages of measurement-level population averaging: First, filters

257  with tuning centers on either side of the vertical meridian were translated separately

258  toward their respective hemifield-specific population averages. Second, a global-pool

259  averaging was performed similarly to the other models. The contribution of these two

260  population-average signals to the measured responses was modeled by 2 additional

261  parameters (Figure 4d). The additional hemifield-specific averaging stage was necessary

262  to account for strong view-specific effects in early visual cortex, but did not materially

263  contribute to the fit in ventral temporal regions.

Figure 4. Schematic illustration of processing stages for the Gabor filter model. (**a**) The model receives gray-scale image intensities for each face exemplar. Three examples input images are illustrated in rows. (**b**) Image intensities are passed through banks of Gabor filters. The banks vary in spatial scale (filter standard deviation and grid spacing). The rows illustrate example filters from each bank. (**c**) The output of each filter bank is weighted and measurement effects are modeled using subsequent hemifield-specific and global-pool population averaging stages (**d**). The final output of the model is a Euclidean distance matrix estimated from the activation vectors in response to each face.

Multiple models can explain cortical and perceptual face spaces

We fitted each of the computational models so as to best predict the

representational distance matrices from cortical regions and perceptual judgments. We

used a leave-one-participant-out cross-validation approach, in which model

performance was evaluated on participants and face identities not used in fitting the

parameters (Experimental Procedures). Model performance was summarized as the

Fisher-Z-transformed Pearson correlation coefficient between the model distances and

the data distances. We performed statistical inference on the average Fisher-Z-

transformed correlations over all train-test splits of the data using t tests. Our cross-

validation scheme tests for generalization across participants and face identities and

ensures that models that differ in complexity (number of free parameters) can be

compared. In order to investigate the effect of local averaging in fMRI voxels on

representational similarity, we fitted two variants of each model: the full model and a

variant that excluded measurement-level population averaging.

We found that all evaluated models explained almost all the explainable variance for

the perceptual face space (Figure 5a), with only negligible differences in cross-validated

generalization performance (for all pairwise model comparisons, see S4 Table). The

inclusion of measurement-level population averaging had little effect on performance.

This is expected because perceptual judgments, unlike fMRI voxels, are not affected by

local averaging across representational units. Thus, the behavioral data was ambiguous

with regard to the proposed models, which motivates model selection by comparison to

the functional imaging data.

Figure 5. Cross-validated generalization performance for computational face-space (green bars) and image-based (orange bars) models, as well as mean performance for fixed predictors (final two bars in each panel). The bars provide group-averaged Pearson correlation coefficients, while individual participants are overlaid in gray markers. Filled bars indicate full model fits, while outlined bars indicate model fits excluding measurement-level population averaging. Statistically significant differences between model variants with and without population averaging are illustrated with black connection lines (p<0.05, see S4 Table for all pairwise comparisons). An estimate of the maximal performance expected given signal-to-noise levels in the sample is illustrated as a shaded noise ceiling (Experimental Procedures). Performance is plotted in separate panels for perceptual judgments (**a**), early visual cortex (**b**), and the fusiform face area (**c**). For other regions of interest, see S5 Figure.

Unlike the perceptual judgments data, the cortical face spaces exhibited substantial

differences between the model fits, with a robust advantage for measurement-level

population averaging in most cases. In the following, we focus on generalization

performance for fits to the early visual cortex and the fusiform face area (for fits to other

regions, see S5 Figure).

The early visual cortex was best explained by the Gabor-filter model, which beat the

alternative computational models (p<0.001 for all pairwise model comparisons, S4

Table) and came close to explaining all explainable variance given noise levels in the

data. Generalization performance for this model was slightly, but significantly better

(p=0.009, Figure 5b) when population averaging was enabled. As a control, we also

tested raw pixel intensities as the representational units. We found no significant

difference in performance between the 0-parameter pixel-intensity model and the fitted

Gabor-filter model with population averaging (p=0.380).

The fusiform face area was also well explained by the Gabor-filter model, but in this

region we observed similar performance for the sigmoidal-ramp-tuning model. Both

models, with population averaging, reached the lower bound of the noise ceiling

(Experimental Procedures; Figure 5c, S4 Table), suggesting that these models were able

to explain the variance in the dataset that was consistent between participants.

Measurement-level population averaging improved generalization performance in the

fusiform face area for both the Gabor-filter (p<0.001) and sigmoidal-ramp-tuning

models (p=0.032), but did not improve either of the exemplar models (p=0.263 for

Gaussian exemplar, p=0.096 for negative Gaussian exemplar). In summary, the

representation in the fusiform face area could be explained by multiple models, and in

most cases measurement-level population averaging improved the quality of the fit.

Regional-mean activation profiles are consistent with sigmoidal-ramp

and Gabor-filter, but not Gaussian-exemplar models

Multiple computational models provided qualitatively similar fits to our cortical data

at the distance-matrix level. However, we might still be able to adjudicate between them

at the level of regional-mean activation profiles. To this end, we obtained activation-

profile predictions from each model by averaging over all model units. We then

correlated the predicted population-mean activation profile with the regional-mean

fMRI activation profile for each participant. Even though these models were fitted to

distance matrices rather than to regional-mean fMRI responses, we found that they

exhibited systematic population-mean response preferences as a function of face-space

eccentricity (Figure 6, for other regions see S6 Figure). In particular, the sigmoidal-ramp

and Gabor-filter models both predicted increasing population-mean responses with

face-space eccentricity, while the Gaussian-exemplar model predicted decreasing

responses with eccentricity (S5 Table, S6 Table for pairwise comparisons). This

constitutes evidence against the Gaussian-exemplar model, under the assumption that

neuronal activity is positively associated with regional-mean fMRI response in visual

regions (29–33). The preference for faces closer to the face-space origin (sub-

caricatures) in the Gaussian-exemplar model arises as a necessary consequence of the

Gaussian distribution of preferred faces, which is centered on the average face. We also

tested a Gaussian exemplar-tuning model with an inverted Gaussian distribution of

preferred faces. In this model, more units prefer faces far from the norm (caricatures)

than faces close to the norm (sub-caricatures). However, the inverted-Gaussian

exemplar model's generalization performance was considerably worse than the

standard-Gaussian exemplar model's (Figure 5).

In summary, exemplar models accurately predicted representational distances for

cortical face spaces when the preferred-face distribution was Gaussian, but such

distributions led to inaccurate predictions of regional-mean fMRI activation profiles.

Thus, analysis of regional-mean fMRI responses enabled us to adjudicate between

models that made similar predictions at the distance-matrix level, and specifically

indicated that the Gaussian exemplar model is unlikely to be the correct model for

cortical face-space representation, despite a good fit at the distance-matrix level.

Figure 6. Activation-profile similarity analysis for computational face-space and image processing models. Bars (panels **a**, **e**) are plotted similarly as in Figure 5, with group-average effects in bars and single-participant estimates in markers. Markers in the line graphs (panels **b-d, f-h**) indicate group-average fMRI responses evoked by each face exemplar, while lines indicate the computational model predictions (with measurement-level population averaging in filled lines, without in outlined lines). Data and model predictions have been Z-scored to better illustrate the correlation-based fit metric we use here. The top panels illustrate effects in the early visual cortex, while the bottom panels illustrate effects in the fusiform face area. For other regions of interest, see S6 Figure.

Measurement-level population averaging is necessary to account for symmetric-view tolerance and over-representation of eccentricity

We found that models that included measurement-level population averaging

generally outperformed models that did not. This advantage appeared to originate in

how models with population averaging captured two effects in the cortical face spaces:

symmetric view-tolerance and over-representation of face-space eccentricity relative to

direction.

First, population averaging enabled the image-based Gabor-filter model to exhibit

symmetric-view-tolerant responses to the face exemplars. Two mirror-symmetric views

will drive a mirror symmetric set of Gabor features. Thus, while the pattern of activity

differs, the population-mean activity is similar. Measurement-level pooling over filters

centered on distinct visual field locations therefore renders symmetric views more

similar in the representation. For instance, the face space in the fusiform face area

exhibited little sensitivity to viewpoint, and the Gabor-filter model fit to this region was

greatly improved by the inclusion of measurement-level population averaging (Figure

5c, S2 Figure). Indeed, with population averaging, generalization performance for the

image-based Gabor-filter model was similar to the sigmoidal-ramp-tuning and exemplar

models, for which view tolerance is assumed at the input stage. General view tolerance,

beyond the symmetric views we used here, is computationally more challenging.

However, for our stimulus set, it was not necessary to posit any intrinsic view-invariant

computations in the fusiform face area to explain how its face spaces come to exhibit

symmetric view tolerance.

Second, measurement-level population averaging increased the degree to which

both the sigmoidal-ramp and the Gabor-filter model over-represented face-space

eccentricity relative to direction, which improved the fit for multiple cortical regions. To

isolate this smaller effect from the larger symmetric-view-tolerance effect, we collapsed

viewpoint in the first-level single-participant fMRI linear model and re-estimated the

cortical face spaces and all model fits for the resulting simplified 12-condition design

matrix, where each predictor coded appearances of a given face identity regardless of its

viewpoint (S7 Figure). Even after collapsing across viewpoints at the first level in this

way, measurement-level population averaging still improved the generalization

performance of the sigmoidal-ramp and the Gabor-filter model in nearly all cases

($p < 0.05$, see S7 Table for descriptive statistics and S8 Table for all pairwise

comparisons), including the early visual cortex ($p < 0.001$ for sigmoidal ramp tuning,

$p = 0.004$ for Gabor filter) and the fusiform face area ($p = 0.001$ for sigmoidal ramp tuning,

$p = 0.007$ for Gabor filter). Thus, the advantage for measurement-level population

averaging could not be accounted for by the fact that it helps explain symmetric view

tolerance. In sum, the addition of population averaging to the model improved model

generalization performance, and this advantage appeared to originate in accounts for

two distinct observed phenomena.

Discussion

This study investigated human face processing by measuring how a face space of individual exemplars was encoded in visual cortical responses measured with fMRI and in perceptual judgments. Relative to a reference PCA model of the 3D shape and texture of faces, cortical face spaces from all targeted regions systematically over-represented eccentricity relative to direction (i.e., the radial relative to the tangential axis). Cortical regions varied in their sensitivity to face viewpoint. We fitted multiple computational models to the data. Considered collectively, the cortical face spaces in the fusiform face area were most consistent with a face-space-based sigmoidal-ramp-tuning model and an image-based Gabor-filter model, and less consistent with models based on exemplar coding. As expected, effects in the early visual cortex were consistent primarily with the Gabor-filter model. In all cases, the winning models' performance depended on the inclusion of a measurement-level population-averaging mechanism, which approximates how individual model units are locally averaged in functional imaging measurements.

Functional MRI responses in the fusiform face area are best explained by sigmoidal-ramp-tuning and Gabor-filter models

Out of the models we considered, the best accounts for the fusiform face area were a face-space-based sigmoidal-ramp-tuning model and an image-based Gabor-filter model. Exemplar-coding models exhibited relatively lower generalization performance, or made inaccurate predictions for regional-mean fMRI activation profiles. Importantly, the advantage for both the sigmoidal-ramp and Gabor-filter model depended on the measurement-level population averaging mechanism. The key contribution of our modeling effort is to narrow the set of plausible representational models for the fusiform face area to two models that can explain both representational distances and the regional-mean activation profile.

It may appear surprising that a face-space coding model based on sigmoidal-ramp

tuning and an image-based model based on Gabor filters should perform so similarly

when fitted to face spaces in the fusiform face area. However, the sigmoidal-ramp-

tuning model captures continuous variation in face shape and texture, which covaries

with low-level image similarity. For instance, local curvature likely increases with face

space eccentricity and is encoded in a ramp-like manner at intermediate stages of visual

processing in macaque V4 (27). Conversely, the Gabor-filter model likely possesses

sensitivity to face-space direction because the contrast of local orientation content

varies with major face features such as eyebrow or lip thickness. There are multiple

ways to parameterize face space, not all of which require domain-specific face features.

This might also clarify why scene-selective areas such as the parahippocampal place

area exhibited somewhat similar representational spaces as face-selective regions in the

current study. Such widely-distributed face-exemplar effects are consistent with

previous decoding studies (2,4). The Gabor-filter model provides one simple account for

how such widely distributed face-exemplar effects can arise. It is likely that the face-

space effects we report are driven at least in part by a general mechanism for object

individuation in visual cortex rather than the engagement of specialized processing for

face recognition.

Symmetric-view tolerance and over-representation of eccentricity in

representational distances can be modeled as an fMRI measurement

effect

The models we evaluate here raise the provocative possibility that in some cases,

fMRI effects that might conventionally be attributed to high-level featural coding could

instead arise from the neuroimaging measurement process. Such an explanation

appears possible for two effects in our data. First, even though the Gabor-filter model is

a single-layer network with limited representational flexibility, this model nevertheless

exhibited near-complete tolerance to mirror-symmetric viewpoint changes, when

coupled with measurement-level population averaging. Second, both this model and the

sigmoidal-ramp-tuning model showed greater over-representation of eccentricity when

measurement-level population averaging was enabled, suggesting that this over-

representation in the fMRI data might also plausibly arise through local averaging in

voxels.

Previous studies have tended to interpret view-tolerant fMRI effects in terms of

cortical processing to support invariant object recognition (2,34,35). The Gabor-filter

model suggests a mechanism by which functional imaging measures can exaggerate

apparent view-tolerance through spatial pooling over neuronal responses. This result

does not contradict previous reports of view-tolerant coding for faces in neuronal

population codes measured with single-unit recording (36–39), but rather

demonstrates that the type of tolerance to symmetric viewpoint changes that we

observed in the current study can be explained without resorting to such intrinsic view-

tolerant mechanisms (see also Ramirez et al. (40)). Such findings may go some way

toward reconciling apparent discrepancies between single-unit and functional imaging

data. For instance, tolerance to symmetrical viewpoints is widespread in human visual

cortex when measured with fMRI (34), but appears specific to a subset of regions in the

macaque face-patch system when measured with single-unit recordings (36). These

results are only contradictory if the measurement process is not considered. In

summary, we demonstrate that measurement effects can produce apparent view

tolerance in fMRI data. This finding does not suggest that fMRI cannot detect view-

tolerant coding (see also 41). For example, population averaging may not account for all

cases of non-symmetric view tolerance. However, our results do suggest that modeling

of the measurement process is important to correctly infer the presence of such

mechanisms from neuroimaging measurements.

Greater regional-mean activation for distinctive faces can arise from local averaging of neuronal responses

The winning models in this study exemplify how sensitivity to face-space eccentricity at the regional-mean activation level can arise as an artifact of averaging, with no individual neuron encoding distinctiveness or an associated psychological construct. Previous functional imaging studies often interpreted response modulations with face eccentricity as evidence for coding of distinctiveness or related social perception attributes (21–23,43). However, both the face-space-based sigmoidal-ramp-tuning model and the image-based Gabor-filter model exhibited increasing population-average responses with eccentricity, even though neither model encodes eccentricity at the level of its units. Although one could, of course, construct a competing model that explicitly codes eccentricity, the models used here are more consistent with single-unit recording studies, where cells generally are tuned to particular features, with a preference for extreme values, rather than responding to eccentricity regardless of direction (20,27,28). Here we demonstrate that when the local averaging of such biologically plausible neuronal tunings is modeled, eccentricity sensitivity emerges without specialized encoding of this particular variable. Related effects have been reported in attention research, where response-gain and contrast-modulation effects at the single-neuron level may sum to similar additive-offset effects at the fMRI-response level (44). In summary, direct interpretation of regional-mean fMRI activations in terms of neuronal tuning can be misleading when the underlying neuronal populations are heterogeneous.

Modeling of measurement-level population averaging is important for computational studies of cortical representation

A simple model of measurement-level population averaging was sufficient here to substantially improve the generalization performance of multiple computational models

for multiple cortical regions. The precise way that fMRI voxels sample neuronal activity

patterns remains a topic of debate (30,31,33,45). A mechanistic model of voxel-sampling

is unlikely to be robustly identifiable at the single-voxel level. However, under the

simple assumption that voxels average random subsets of neurons with nonnegative

weights, the effect on the apparent representational geometry will be a uniform

stretching along the all-one vector (representing the population average). Here we

approximated this effect for models with nonlinear parameters by mixing the

population average into the predicted representational feature space. Despite the

simplicity of this method, our noise-ceiling estimates indicate that the winning models

captured nearly all the explainable variance in the current dataset. For model

representations without nonlinear parameters, this measurement model can be

implemented more easily by linearly combining the model's original distance matrix and

the distance matrix obtained for the population average dimension of the space (using

squared Euclidean distances estimates, see also 46–48). Thus, the measurement-level

population averaging mechanism we propose here is widely and easily applicable to any

case where a computational model is compared to neuroimaging data at the distance-

matrix level.

The distance-matrix effects of local pooling of neuronal responses in fMRI voxels is

correctly accounted for by our measurement model under the assumption that neurons

are randomly intermixed in cortex (i.e. voxels sample random subsets of neurons). This

simplifying assumption is problematic for early visual areas, where there is a well-

established retinotopic organization with a strong contralateral response preference.

For the retinotopic Gabor filter model, we therefore added a hemifield-specific pooling

stage, which helped account for strong view-sensitivity in occipital regions of interest.

Accounting for measurement effects in the presence of topographic organization is likely

to prove more challenging for naturalistic stimulus sets. One solution is to account for

local averaging in fMRI voxels by local averaging of the model's internal

representational map (42). This local-pooling approach can be thought of as providing a

further constraint on the comparison between model and data, because smoothing the

model representation is only expected to improve the fit if the model response

topography resembles the cortical topography. This may provide a means of

adjudicating between topographically organized models, even when the models predict

similar distance matrices in the absence of measurement-effect modeling. In summary,

the global population average is a special dimension of the representational space,

which is overrepresented in voxels that pool random subsets of neurons. This effect

accounts for much variance in the representational distances in the current study, and is

easy to model. Modeling the overrepresentation of the global average, as we did here, is

suitable for models that do not predict a spatial organization (e.g. face-space coding

models). For models that do predict a spatial organization, it may be more appropriate

to simulate fMRI voxels by local averaging of the model's representational map (42).

Model comparison is essential for computational neuroimaging

This study demonstrates the importance of considering multiple alternative models

to guide progress in computational neuroimaging. In particular, the finding that

practically every model we evaluated exhibited significantly greater-than-zero

generalization performance strongly suggests how studies that only evaluate a limited

set of candidate models can arrive at misleading conclusions (see e.g. 49).

Although the central goal of model comparison is to select the best account of the

data, the finding that some models are not dissociable under the current experimental

context also has important implications for the design of future studies. Here we

demonstrated that Gaussian-distributed exemplar-coding models are less likely to

account for human face coding, while accounts based on sigmoidal ramp tuning and

Gabor filter outputs perform very similarly. This suggests the need to design stimulus

sets that generate distinct predictions from these winning models. For example,

presenting face stimuli on naturalistic textured backgrounds may be sufficient to

adjudicate between the two models, because the Gabor-filter model lacks a mechanism

for figure-ground separation. In conclusion, our study exemplifies the need to test and

compare multiple models and suggests routes by which the sigmoidal-ramp-tuning

model of face-space coding could be further evaluated.

Materials and Methods

Data and software availability

The distance matrices we estimated for cortical and perceptual face spaces are available, along with software to re-generate all computational model fits (separate copies deposited on https://osf.io/5g9rv; https://doi.org/10.5281/zenodo.242666).

Sampling the reference PCA face space

We generated faces using a norm-based model of 3D face shape and texture, which has been described in detail previously (15,25). Briefly, the model comprises two PCA solutions (each trained on 200 faces), one based on 3D shape estimated from laser scans and another based on texture estimated from digital photographs. The components of each PCA solution are considered dimensions in a space that describes natural variation in facial appearance. All stimulus generation was performed using the PCA solution offered by previous investigators, and no further fitting was performed for this study. We yoked the shape and texture solutions in all subsequent analyses since we did not have distinct hypotheses for these.

We developed a method for sampling faces from the reference PCA space in a manner that would maximize dissimilarity variance. This is related to the concept of design efficiency in univariate general linear modeling (51), and involves maximizing the variance of hypothesized distances over the stimulus set. Because randomly sampled distances in high dimensional spaces tend to fall in a narrow range of distances relative to the norm (52), we reduced each participant's effective face space to 2D by specifying a plane which was centered on the norm of the space and extended at a random orientation. The face exemplars constituted a polar grid on this plane, with 4 directions at 60 degrees separation and 3 eccentricity levels (scaled at 30%, 100% and 170% of the mean eccentricity in the training face set). The resulting half-circle grid on a

plane through the high-dimensional space is adequate for addressing our hypotheses

concerning the relative role of direction and eccentricity coding under the assumption

that the high-dimensional space is isotropic. The orientation of the face-space slice was

randomized between participants and model fits were based on cross-validation over

participants. Under these conditions, any non-isotropicity is only expected to impair

generalization performance. In preliminary tests we observed that this method yielded

substantially greater dissimilarity variance estimates than methods based on Gaussian

or uniform sampling of the space.

Face animation preparation

We used Matlab software to generate a 3D face mesh for each exemplar. This mesh

was rendered at each of the orientations of interest in the study in a manner that

centered the axis of rotation on the bridge of the nose for each face. This procedure

ensured that the eye region remained centered on the fixation point throughout each

animation in order to discourage eye movements. Renders were performed at sufficient

increments to enable 24 frames per second temporal resolution in the resulting

animations. Frames were converted to gray-scale and cropped with a feathered oval

aperture to standardize the outline of each face and to remove high-contrast mesh edges

from the stimulus set. Finally, we performed a frame-by-frame histogram equalization

procedure where the average histogram for each frame was imposed on each individual

face. Thus, the histogram was allowed to vary across time but not across faces. Note that

histogram matching implies that the animations also have identical mean gray-scale

intensity and root-mean-square contrast.

A potential concern with these matching procedures is that they could affect the

validity of the comparison to the reference PCA space. However, we found that the

opposite appeared to be true: distances in the reference PCA space were more

predictive of pixelwise correlation distances in the matched images than in the original

images. Thus, the matching procedure did not remove features that were encoded in the

PCA space and may in fact have acted to emphasize such features.

Participants

10 healthy human participants participated in a similarity judgment task and fMRI

scans. The psychophysical task comprised 4 separate days of data collection which were

completed prior to 4 separate days of fMRI scans. All procedures were performed under

a protocol approved by the Cambridge Psychology Research Ethics Committee (CPREC).

Participants were recruited from the local area (Cambridge, UK) and were naïve with

regard to the purposes of the study. Five additional participants participated in initial

data collection but were not invited to complete the study due to difficulties with

vigilance, fixation stability, claustrophobia and/or head movements inside the scanner.

The analyses reported here include all complete datasets that were collected for the

study.

Perceptual similarity judgment experiment

We used a pair-of-pairs task to characterize perceptual similarity (S1 Movie).

Participants were presented with two vertically offset pairs of faces on a standard LCD

monitor under free viewing conditions, and judged which pair was relatively more

dissimilar with a button press on a USB keyboard (two-alternative force choice). Each

face rotated continuously between a leftward and a rightward orientation (45 degrees

left to 45 degrees right of a frontal view over 3 seconds). Ratings across all possible

pairings of face pairs (2145 trials: all pairings of the 66 possible pairs of the 12 faces)

were combined into a distance matrix for each participant, where each entry reflects the

percentage of trials on which that face pair was rated as relatively more dissimilar.

Functional MRI experiment

We measured brain response patterns evoked by faces in a rapid event-related fMRI experiment (S2 Movie). Participants fixated on a central point of the screen where a pseudo-random sequence of face animations appeared (7 degrees visual angle in height, 2s on, 1s fixation interval). We verified fixation accuracy online and offline using an infrared eye tracking system (Sensomotoric Instruments, 50Hz monocular acquisition). The faces rotated outward in leftward and rightward directions on separate trials (18 to 45 degrees rotation left or right of a frontal view), and participants responded with a button press to occasional face repetitions regardless of rotation (one-back task). This served to encourage attention to facial identity rather than to incidental low-level physical features. Consistent with a task strategy based on identity recognition rather than image matching, participants were sensitive to exemplar repetitions within viewpoint (mean d'+-1 standard deviation 2.68+-0.62) and to exemplar repetitions where the viewpoint changed (2.39+-0.52).

The experiment was divided into 16 runs where each run comprised 156 trials bookended by 10s fixation intervals. Each scanner run comprised two experimental runs, which were modeled independently in all subsequent analyses. The trial order in each run was first-order counterbalanced over the 12 faces using a De Bruijn sequence (53) with 1 additional repetition (diagonal entries in transfer matrix) added to each face in order to make the one-back repetition task more engaging and to increase design efficiency (51). The rotation direction in which each face appeared was randomized separately, since a full 24-stimulus De Bruijn sequence would have been over-long (576 trials). Although the resulting 24-stimulus sequences were not fully counter-balanced, we used an iterative procedure to minimize any inhomogeneity by rejecting rotation direction randomizations that generated off-diagonal values other than 0 and 1 in the 24-condition transfer matrix (that is, each possible stimulus-to-stimulus transfer in the sequence could appear once or not at all). These homogeneous trial sequences served to

enhance cross-validation performance by minimizing over-fitting to idiosyncratic trial

sequence biases in particular runs. We modeled the data from each run with one

predictor per face exemplar and viewpoint.

Magnetic resonance imaging acquisition

Functional and structural images were collected at the MRC Cognition and Brain

Sciences Unit (Cambridge, UK) using a 3T Siemens Tim Trio system and a 32-channel

head coil. Functional runs used a 3D echoplanar imaging sequence (2mm isotropic

voxels, 30 axial slices, 192 x 192mm field of view, 128 x 128 matrix, TR=53ms,

TE=30ms, 15° flip angle, effective acquisition time 1.06s per volume) with GRAPPA

acceleration (acceleration factor 2 x 2, 40 x 40 PE lines). Each participant's functional

dataset (7376 volumes over 8 scanner runs for the main experiment) was converted to

NIFTI format and realigned to the mean of the first session's first experimental run

using standard functionality in SPM8 (fil.ion.ucl.ac.uk/spm/software/spm8/). A

structural T1-weighted volume was collected in the first session using a multi-echo

MPRAGE sequence (1mm isotropic voxels)(54). The structural image was de-noised

using previously described methods (55), and the realigned functional dataset's header

was co-registered with the header of the structural volume using SPM8 functionality.

The structural image was then skull-stripped using the FSL brain extraction tool

(fmrib.ox.ac.uk/fsl), and a re-sliced version of the resulting brain mask was applied to

the fMRI dataset to remove artifacts from non-brain tissue. We constructed design

matrices for each run of the experiment by convolving the onsets of experimental events

with the SPM8 canonical hemodynamic response function. Slow temporal drifts in MR

signal were removed by projecting out the contribution of a set of nuisance trend

regressors (polynomials of degrees 0-4) from the design matrix and the fMRI data in

each run.

Cross-validated discriminant analysis

We estimated the neural discriminability of each face pair for each region of interest

using a cross-validated version of the Mahalanobis distance (56). This analysis improves

on the related Fisher's linear discriminant classifier by providing a continuous metric of

discriminability without ceiling effects. Similarly to the linear discriminant, classifier

weights were estimated as the contrast between each condition pair multiplied by the

inverse of the covariance matrix of the residual time courses, which was estimated using

a sparse prior (57). This discriminant was estimated separately for the concatenated

design matrix and fMRI data in each possible leave-one-run-out training split, and the

resulting weights were transformed to unit length and projected onto the contrast

estimates from each training split's corresponding test run (16 estimates per contrast).

The 16 run-specific distance estimates were averaged to obtain the final neural

discriminability estimate for that participant and region. When the same data is used to

estimate the discriminant and evaluate its performance, this algorithm returns the

Mahalanobis distance, provided that a full rather than sparse covariance estimator is

used (56). However, unlike a true distance measure, the cross-validated version that we

use here is centered on 0 under the null hypothesis. This motivates summary-statistic

random-effects inference for above-chance performance using conventional T tests.

We developed a variant of this discriminant analysis where effects that might be

broadly described as region-mean-related are removed (S4 Figure). This control

analysis involved two modifications to how contrasts were calculated at the level of

forming the discriminant and at the level of evaluating the discriminant on independent

data. First, each parameter estimate was set to a mean of zero in order to remove any

additive offsets in response levels between the conditions. Second, for each pair of

mean-subtracted parameter estimates, the linear contribution of the mean estimate

over the pair was removed from each estimate before calculating the contrast. This

corrects for the case where a single response pattern is multiplicatively scaled by the

conditions. The resulting control analysis is insensitive to effects driven by additive or

multiplicative scaling offsets between the conditions.

Multiple regression RSA

We used a multiple regression model to estimate the relative contribution of

eccentricity and direction to cortical and perceptual face-space representations.

Multiple regression fits to distance estimates can be performed after a square transform,

since squared distances sum according to the Pythagorean theorem. We partitioned the

squared distances in the reference PCA space into variance associated with eccentricity

changes by creating a distance matrix where each entry reflected the minimum distance

for its eccentricity group in the squared reference PCA matrix (that is, cases along the

group's diagonal where there was no direction change). The direction matrix was then

constructed as the difference between the squared reference PCA matrix and the

eccentricity matrix (Figure 2a). These predictors were vectorized and entered into a

multiple regression model together with a constant term. This partitioning of the

dissimilarity variance in the reference PCA matrix is complete in the sense that a

multiple regression RSA model where the reference PCA matrix is used as the

dependent variable yields parameter estimates of [1,1,0] for eccentricity, direction and

constant, respectively, with no residual error. These three predictors were then split

according to viewpoint, with separate sets of predictors for distances within and across

viewpoint. The absolute values of the cortical and perceptual distance matrices were

squared and then transformed back to their original sign before being regressed on the

predictor matrix using ordinary least squares. Finally, the absolute values of the

resulting parameter estimates were square-root transformed and returned to their

original signs.

Functional regions of interest

We used a conventional block-based functional localizer experiment to identify category-selective and visually-responsive regions of interest in human visual cortex. Participants fixated a central cross on the screen while blocks of full-color images were presented (36 images per block presented with 222ms on, 222ms off, 16 s fixation). Participants were instructed to respond to exact image repetitions within the block. Each run comprised 3 blocks each of faces, scenes, objects and phase-scrambled versions of the scene images. Each participant's data (8 runs of 380 volumes) was smoothed with a Gaussian kernel (6mm full width at half maximum) and responses to each condition were estimated using a standard SPM8 first-level model. Regions of interest were identified using a region-growing approach, where a peak coordinate for each region was identified in individual participants, and a region of interest was grown as a contiguous set of the most selective 100 voxels extending from this coordinate. We defined the face-selective occipital and fusiform face areas with the minimum-statistic conjunction contrast of faces over objects and faces over baseline, and the scene-selective parahippocampal place area and transverse occipital sulcus as the minimum-statistic conjunction contrast of scenes over objects and scenes over baseline, and the early visual cortex as the contrast of scrambled stimuli over the fixation baseline. We also attempted to localize a face-selective region in the posterior superior temporal sulcus, a face-selective region in anterior inferotemporal cortex and a scene-selective region in retrosplenial cortex, but do not report results for these regions here since they could only be identified in a minority of the participants. All regions of interest were combined into bilateral versions before further analysis since we did not have distinct predictions concerning functional lateralization.

Sigmoidal ramp tuning model

The sigmoidal ramp model comprises 1000 model units, each of which exhibits a

monotonically increasing response in a random direction extending from the origin of

the face space (Figure 3). The response y at position x along the preferred direction is

described by the sigmoid

y[raw] = 1 / (1+exp((-x+o)/s));

where the free parameters are o, which specifies the horizontal offset of the

response function (zero places the midpoint of the response function at the norm of the

space, values greater than zero corresponds to responses shifted away from the norm),

and s, which defines response function saturation (4 corresponds to a near-linear

response in the domain of the face exemplars used here, while values near zero

correspond to a step-like increase in response). The raw output of each model unit is

then translated toward the population-mean response

y[final] = (y[raw]-y[mean]) * (1-p) + y[mean]

where p is a free parameter that defines the strength of measurement-level

population averaging (0 corresponds to no averaging, 1 corresponds to each model unit

returning the population-mean response).

Exemplar model

The exemplar model comprises 1000 model units, each of which prefers a Cartesian

coordinate in the face space with response fall-off captured by an isotropic Gaussian.

The free parameters are w, which controls the full width at half-maximum tuning width

of the Gaussian response function, and d, which controls the width of the Gaussian

distribution of tuning centers (0.1 places Z=2.32 at 10% of the eccentricity of the

caricatures while 3 places this tail at 300% of the eccentricity of the caricatures).

We also constructed an inverted-Gaussian variant of this model where the

distribution of distances was inverted at Z=2.32 and negative distances truncated to

zero (1% of exemplars). This model was fitted with similar parameters as the original

Gaussian exemplar model.

Gabor filter model

The Gabor filter model is an adaptation of a neuroscientifically-inspired model that

has previously been used to successfully predict single-voxel responses in the early

visual cortex (24, github.com/kendrickkay/knkutils/tree/master/imageprocessing).

The model is composed of 5 banks of Gabor filters varying in spatial position, phase (2

values) and orientation (8 directions, Figure 4). We measured each filter's response to

the last frame of each animation, and corrected for phase shifts. The resulting rectified

response vectors were weighted according to filter bank membership (5 free

parameters). We estimated measurement-level population averaging using two pooling

stages: a hemifield-specific pool, where filters were pooled according to whether their

centers fell left or right of the vertical meridian, followed by a global pool.

Pixelwise correlation predictor

We used a fixed control predictor to estimate whether coding based on pixelwise

features would produce the same face space warping we observed in our data (Figure

4). The pixelwise correlation predictor was generated by stacking all the pixels in each

of the face animations into vectors and estimating the correlation distance between

these intensity values.

Estimating the noise ceiling

We estimated the noise ceiling for Z-transformed Pearson correlation coefficients

based on methods described previously (56). This method estimates the explained

variance that is expected for the true model given noise levels in the data. Although the

true noise level of the data cannot be estimated, it is possible to approximate its upper

and lower bounds in order to produce a range within which the true noise ceiling is

expected to reside. The lower bound estimate is obtained by a leave-one-participant-out

cross-validation procedure where the mean distance estimates of the training split are

correlated against the left-out-participant's distances, while the upper bound is obtained

by performing the same procedure without splitting the data. These estimates were

visualized as a shaded region in figures after reversing the Z-transform (Figure 4).

Statistical inference

All statistical inference was performed using T-tests at the group-average level

(N=10 in all cases except the occipital face area and transverse occipital sulcus, N=9).

Correlation coefficients were Z-transformed prior to statistical testing. Average Z

statistics were reverse-transformed before visualization for illustrative purposes.

Fold-wise generalization performance estimates are partially dependent, which can

lead to sample variance underestimates (58,59) and greater than intended false positive

rates when conventional parametric statistics are used. However, we simulated the

effects of this potential bias and found no consistent inflation in false-positive rates for

simulations of the parameters used in the current study (S1 Code, S8 Figure, S9 Figure).

Thus, the inferential statistics reported in the current study appear to be robust to this

slight dependence and maintain their intended frequentist properties.

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1009

1010 ***Supporting information***

Figure S1

1011

S1 Figure. Example stimulus sets for 4 participants. Each stimulus set shares the

same underlying distance matrix in the reference PCA space, while the randomization of

the orientation of the plane on which the faces are sampled ensures that each set is

visually distinct.

S2 Figure. Group-average distance matrices from additional regions of interest and

best-fitting model predictions from each model considered in the main manuscript

(Figure 5).

1020

S3 Figure. Cortical direction discriminability as a function of eccentricity level. Each

point reflects the mean performance for all directions at a given eccentricity level (4x4

block diagonals in Figure 1) for a single participant. Small random offsets have been

added to each x coordinate for illustrative purposes, and a line shows the least-squares

fit. Performance is plotted separately for distances within viewpoint (round markers,

solid line, left offset) and across viewpoint (square markers, dashed line, right offset). All

plotted p values are obtained through group analysis of single-participant estimates.

Within viewpoint, cortical discrimination performance increases with eccentricity level

in all regions except the parahippocampal place area (e). Across viewpoint, statistically

significant effects are observed in the ventral temporal fusiform face area in the lateral

temporal transverse occipital sulcus, but not in occipital areas (early visual cortex,

occipital face area).

1033

1034   *S4 Figure.* Effect of region-mean removal on cortical face spaces. The top row shows

1035   original distance matrices, while the bottom row shows distance matrices after

1036   removing additive and multiplicative mean pattern effects (Experimental Procedures).

1037   The cited Pearson correlation coefficients are calculated at the group-average level.

1038

1039   *S5 Figure*. Cross-validated distance-matrix generalization performance for

1040   additional cortical regions of interest. Plotted as Figure 5 in main text.

1041

1042   *S6 Figure*. Cross-validated activation-profile generalization performance for

1043   additional cortical regions of interest. Plotted as in Figure 6 in main text.

1045 *S7 Figure.* Cross-validated distance-matrix similarity, data distance matrices and

1046 best-fitting predicted matrices for an analysis where the two viewpoints have been

1047 collapsed into a single set of 12 conditions. Plotted as in Figures 1 and 5 in main text.

1048

S8 Figure. Rejection probability simulation. We simulated out-of-sample

generalization performance for two arbitrary models, using methods that closely

matched the ones described in this manuscript (for details, see S1 Code). We estimated

potential bias by comparing cross-validated generalization performance (panels in

leftmost column) with generalization to a withheld validation set (left column,

subtraction in right column). The probability of rejecting the null hypothesis (p<0.05, T

test) over 100000 simulations is plotted for tests of either model against zero (one-

tailed test, first two rows of panels), and of zero difference between the models'

generalization performance (two-tailed test, bottom row). Each color-mapped image

shows the rejection probability as a function of signal level for model 1 (vertical axis)

and model 2 (horizontal axis). The null hypothesis case is highlighted with white circles.

The bars in the rightmost panel summarize the mean rejection probabilities (ie, false

positives) for each of these null cases.

1062

S9 Figure. Summary plot of the data in Figure S8. Each point represents the mean

rejection probability for a unique set of simulation parameters (values in color-mapped

images in S8 Figure). It can be seen that there is a close to unit relationship between

rejection probability in the dependent, cross-validated case (vertical axis) and the

independent, validation case (horizontal axis).

S1 Code. Code to reproduce S8 Figure and S9 Figure. Requires Matlab R2013a.

S1 Table. Descriptive and inferential statistics for the distance-matrix correlation

between the face-space models the perceptual and cortical face spaces. We report the

group-average correlation coefficient (mean_r), the group-average Z-transformed

correlation (mean_zr), standard error for the Z-transformed correlation (sterr_zr), one-

tailed p values for the Z-transformed correlation (ppara_zr) and sample sizes (n).

Related to Figure 5.

S2 Table. Analysis of variance on parameter estimates from multiple regression RSA

model, with the factors metric (eccentricity, direction), viewpoint (within, across), and a

two-way interaction term. For details, see main text. Related to Figure 2.

S3 Table. Descriptive and inferential statistics for the analysis of direction

discriminability as a function of eccentricity level. Mean, standard error (sterr), one-

tailed p values (ppara) and sample sizes (n) are included on separate rows. See also S3

Figure.

S4 Table. Two-tailed parametric p values for all pairwise comparisons between

model distance-matrix generalization performances (S1 Table). Related to Figure 5.

S5 Table. Descriptive and inferential statistics for activation-profile similarity

analysis. See S1 Table for an account of what the row labels represent. Related to Figure

6.

S6 Table. Two-tailed parametric p values for all pairwise comparisons between

activation-profile model fits (S5 Table). Related to Figure 6.

S7 Table. Descriptive and inferential statistics for collapsed-view distance-matrix

generalization performances. See S1 Table for an account of what the row labels

represent. Related to S7 Figure.

S8 Table. Two-tailed parametric p values for all pairwise comparisons between

collapsed-view distance-matrix generalization performances. See S7 Table, S7 Figure.

S1 Movie. Cropped screen capture of the perceptual judgment task as it appeared to

participants during data collection.

S2 Movie. Cropped screen capture of the main experiment as it appeared to

participants during data collection.