

1 **Online control of prehension predicts performance on a standardised motor**
2 **assessment test in 8-12 year-old children**

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4 **Caroline C.V. Blanchard¹, Hannah L. McGlashan¹, Blandine French¹, Rachel J.**
5 **Sperring², Bianca Petrocochino², & Nicholas P. Holmes¹**

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8 ¹ School of Psychology, University of Nottingham, University Park, Nottingham NG7 2RD, UK

9 ² School of Psychology and Clinical Language Sciences, University of Reading, Reading
10 RG6 6AL, UK

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12 **Corresponding author:** Nicholas P. Holmes

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14 **Running head:** Online control predicts children's aiming and catching

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20 **Abstract**

21 Goal-directed hand movements are guided by sensory information and may be adjusted
22 'online', during the movement. If the target of a movement unexpectedly changes position,
23 trajectory corrections can be initiated in as little as 100ms in adults. This rapid visual online
24 control is impaired in children with developmental coordination disorder (DCD), and
25 potentially in other neurodevelopmental conditions. We investigated the visual control of
26 hand movements in children in a 'centre-out' double-step reaching and grasping task, and
27 examined how parameters of this visuomotor control co-vary with performance on
28 standardised motor tests often used with typically and atypically developing children. Two
29 groups of children aged 8-12 years were asked to reach and grasp an illuminated central ball
30 on a vertically oriented board. On a proportion of trials, and at movement onset, the
31 illumination switched unpredictably to one of four other balls in a centre-out configuration
32 (left, right, up, or down). When the target moved, all but one of the children were able to
33 correct their movements before reaching the initial target, at least on some trials, but the
34 latencies to initiate these corrections were longer than those typically reported in the adult
35 literature, ranging from 211 to 581 ms. These later corrections may be due to less developed
36 motor skills in children, or to the increased cognitive and biomechanical complexity of
37 switching movements in four directions. In the first group (n=187), reaching and grasping
38 parameters significantly predicted standardised movement scores on the MABC-2, most
39 strongly for the aiming and catching component. In the second group (n=85), these same
40 parameters did not significantly predict scores on the DCDQ-07 parent questionnaire. Our
41 reaching and grasping task provides a sensitive and continuous measure of movement skill
42 that predicts scores on standardized movement tasks used to screen for DCD.

43

44 **Introduction**

45 Almost from the moment able-bodied people wake up, they begin reaching and grasping for
46 objects with their hands – bed covers, a cup of coffee, a toothbrush. Coordinating and
47 controlling accurate, goal-directed reaching and grasping movements is done many times a
48 day. Visually-guided movements longer than about 100ms in duration may benefit from
49 visual online control (Castiello et al., 1991; Farnè et al., 2003; Paulignan et al., 1991a,b;
50 Tresilian, 2012) which is the ability to quickly and accurately correct one's movement in
51 response to unexpected changes in the hand or target's position or orientation, for example,
52 when grasping an object as it is falling from your desk (Ruddock et al., 2014). In such
53 situations, the reaching movement must be altered online, to reduce the error and bring the
54 hand and target closer together. This online error correction occurs for many goal-directed
55 movements, but takes some time. The most rapid movement corrections in adult humans
56 begin at 90-120ms after an unexpected change in target object position (Paulignan et al.,
57 1991a); the movement towards the initial target must be cancelled, and an acceleration
58 towards the new target must be programmed. Adjustments to the reaching component of
59 prehension (i.e., hand position) based on changes in object position occur more rapidly than
60 adjustments to the grasping component (hand orientation and grip aperture) based on
61 changes in object size (Paulignan et al., 1991a,b).

62
63 Visual online control is an important part of theories of motor control in which limb
64 movements are controlled by internal feedback loops, which are continuously updated to
65 adjust for error and changes in the environment (Goodale et al., 1986; Hyde and Wilson,
66 2011a, 2011b, Paulignan et al., 1991a, 1991b; Prablanc and Martin, 1992; Wilson et al.,
67 2013). The feedback loops integrate sensory input and motor output to adjust the ongoing
68 motor commands. A review of internal feedback models suggests that accurate arm
69 movements cannot be executed purely under feedback control because visual feedback
70 loops are too slow (Wolpert et al., 1998). Instead, internal models of the body in the brain
71 allow for 'forward' predictions of the likely sensory consequences of ongoing actions so that

72 these likely consequences can be taken into account when correcting movements, in
73 advance of actual feedback.

74
75 In experimental settings, online movement corrections can be studied using a 'double-step'
76 perturbation task, which involves the participant rapidly changing their movement from one
77 target towards another target location (after a 'perturbation' of the target position) before the
78 initial movement is complete (Hyde and Wilson, 2011a; Paulignan et al., 1991a, 1991b;
79 Prablanc and Martin, 1992; Van Braeckel et al., 2007). Wilson and Hyde (2013) used a
80 double-step reaching task to explore age-related changes in visual online control in children.
81 They found that older and mid-aged typically developing (TD) children corrected their
82 reaching during the perturbed trials of the task significantly faster than younger children.
83 They also found that adults were faster than older children on all measures.

84
85 This double-step reaching experimental paradigm has also been used to explore visual
86 online control in children with developmental coordination disorder (DCD, Hyde and Wilson,
87 2011a, 2011b, 2013; Plumb et al., 2008). DCD, sometimes referred to as developmental
88 dyspraxia, or just dyspraxia, is a complex neurodevelopmental disorder and has a
89 prevalence of around 6% in school-age children (American Psychiatric Association, 2000).
90 The DSM-5 diagnostic criteria for DCD includes the disturbances in acquisition and
91 execution of basic motor skills, to the extent that it interferes with daily activities and impacts
92 the child's life both at school and during their leisure time, with an early onset during the
93 developmental period, and that can't be better explained by any other disability (American
94 Psychiatric Association, 2013). Plumb and colleagues (2008) conducted the first study
95 exploring visual online control in children with DCD and did not find evidence for children
96 with DCD having a specific disruption in this domain. However, the authors cautiously noted
97 that performance in their sample was globally so poor that it was not possible to determine
98 where the deficit lay. Instead they supported a more fundamental movement dysfunction that
99 makes it very difficult to pinpoint a specific mechanism. In Plumb and colleagues' study,

100 children stood up and made an aiming movement using a stylus towards a target which
101 changed location unexpectedly on some trials. As they had difficulty performing the task
102 standing, children with DCD were allowed to sit down during the task, and the hand-held
103 stylus was made thicker for them than for the TD children. Plumb and colleagues' results
104 showed that children with DCD took longer to complete the task overall, but there was no
105 significant interaction between condition (perturbation versus non-perturbation) and group
106 (DCD versus TD). As the authors stated, the ability to adjust to perturbations might be
107 related to the quality of motor commands and/or to the quality of the feedback controller.
108 Thus, observing difficulties with visual online control doesn't necessarily imply problem
109 entirely at the level of the feedback controller. However, since the procedure was different for
110 the TD children and children with DCD, the absence of evidence for specific deficits in visual
111 online control was later re-assessed (Hyde and Wilson, 2011a).

112
113 Evidence in support of specific deficits in online control in children with DCD comes from
114 later studies (Hyde and Wilson, 2011a, 2011b; Wilson and Hyde, 2013). Hyde and Wilson
115 (2011a) used a computerised visual online control task, with targets displayed on a LCD
116 touch-screen. Children had electromagnetic sensors attached to their index finger, via a
117 glove, that recorded its position. The authors found that children with DCD displayed longer
118 movement times and increased error rates when responding to target perturbations during
119 the visual online control task. They also found that the performance of children with DCD
120 aged eight to twelve years old was equal to that of typically developing five to seven-year-old
121 children, in regards to rapid online control (Wilson and Hyde, 2013).

122
123 The foregoing work on online control has compared groups of children with DCD to TD
124 children, but has not examined how children's visual online control across a wide range of
125 movement skills covaries with performance on the standardised tests of movement
126 coordination. By testing children both with and without motor impairments, and by assessing
127 a wide range of movement variables on a continuous scale, the present study explores

128 which reaching and grasping parameters best predict scores on standardised measures of
129 movement ability often used for assessing children with DCD - the Movement Assessment
130 Battery for Children 2nd Edition (MABC-2; Henderson, S.E. et al., 2007), and the
131 Developmental Coordination Disorder Questionnaire (DCDQ'07; Wilson et al., 2000, 2009).

132

133 As well as assessing performance across a continuous scale of movement skill, our work is
134 based on a double-step reaching-and-grasping task, involving four alternative possible
135 movement directions, in contrast to the typical two alternative targets used in many prior
136 studies (though see, e.g., Prablanc and Martin, 1992). This more unpredictable displacement
137 of the target object is more like a real-world problem, and reduces both the potential over-
138 learning of a small number of target locations, and the usefulness of movement strategies
139 such as 'reach midway between the targets, then wait to see if anything changes'. Further,
140 instead of presenting targets on a flat, 2D computer screen, which may result in motion blur
141 and a lack of reliable and precise onsets and offsets of the displayed stimuli (Elze and
142 Tanner, 2012), we used LEDs to illuminate, with millisecond precision, translucent table
143 tennis ball targets that were physically grasped by the children. Our aim here is to examine
144 in detail the relationships between visual online control and standardised movement scores
145 in children aged 8-12 years, across a wide range of movement coordination skill.

146

147 **Material and Methods**

148 **Participants**

149 A total of 299 children were studied. After removal of 48 datasets because of electromagnetic
150 artefacts and other outliers (Figure 2), 187 children performed the reaching and grasping
151 task and the MABC-2 (109 females, mean \pm SD age = 9.30 \pm 0.74 years), and 85 children
152 (46 females, mean \pm SD age = 10.34 \pm 0.95 years) participated as part of Nottingham
153 University's public Summer Scientist Week, 2015. For these children, the parents had
154 completed the DCDQ'07 questionnaire. The children were recruited in different ways,
155 including through their teachers, using a local database of schools, directly through parents

156 or caregivers using a local database of individual participants, or by other means (e.g., by
157 their expressing an interest directly or by email during or after outreach work). All the
158 children had normal or corrected vision. All parents and children gave written, informed
159 consent and assent, respectively. The experimental procedures were approved by the local
160 ethical review committees at the Universities of Nottingham and Reading, and were in
161 accordance with the Declaration of Helsinki (as of 2008).

162

163

INSERT TABLE 1 ABOUT HERE

164

165 **Motor and cognitive skills assessment procedures**

166 **Movement Assessment Battery for Children, 2nd Edition** (Henderson et al., 2007) – The
167 MABC-2 is a standardised test used to assess motor coordination impairments in children
168 and adolescents. Children directly perform a set of eight tasks among three components,
169 with three tasks assessing manual dexterity, two assessing aiming and catching, and three
170 assessing balance. Although the skills tested are the same for all, different tasks are
171 designed for three specific age bands: age band 1 (3-6 years), age band 2 (7-10 years) and
172 age band 3 (11-16 years). Each raw score obtained by a child in each of the eight tasks is
173 then converted into an item standard score following a scoring table depending on the child's
174 age within the age band (i.e., for age band 2, 7:0-7:11, 8:0-8:11, 9:0-9:11, 10:0-10:11). These
175 scores are summed into a component score, then converted into standard scores (mean=10,
176 SD=3) with their equivalent percentiles for the three component scores and the total of the
177 MABC-2. To facilitate calculation of standard and component scores, we created macros in
178 Excel to automate this process by extracting the appropriate scores from look-up tables
179 (Supplementary data). In the current study, the tasks were age-appropriate, with all children
180 performing tasks from the 7-10 year old bracket (several children over 10 years of age were
181 tested only with the DCDQ'07, and not with the MABC-2).

182

183 **DCDQ'07** (Wilson et al., 2000, 2009) – The DCDQ'07 is a brief parent questionnaire
184 designed to screen for motor problems associated with DCD in children aged 5 to 15 years.
185 Parents are asked to compare their child's motor performance to that of his/her peers
186 depending on the child age band (5:0-7:11, 8:0-9:11, 10:0-15:0). The DCDQ'07 consists of
187 15 items grouped into 3 areas: control during movement, fine motor/handwriting, and general
188 coordination. For children aged 8 to 10 years, a score of 15-55 suggests the kinds of motor
189 problems associated with DCD, whereas a score of > 55 probably does not indicate such
190 problems. For children aged 10 to 15 years, a score of 15-57 suggests motor problems
191 associated with DCD, where as a score of > 57 probably does not.

192
193 **Online control measure** – We used a centre-out double-step reaching and grasping task to
194 measure how children alter their movement when reaching to grasp an illuminated ball with
195 their dominant hand. Children were seated comfortably at a table with a vertical (40x50 cm)
196 board on the table 30 cm in front of their hand, which was placed on a starting position, 30
197 cm from the board. Five translucent orange table tennis balls (4 cm diameter) were attached
198 at the centre, top, bottom, right and left sides of the board, with the centres of the four
199 eccentric balls 11.5 cm away from the centre (Figure 1).

200

201

INSERT FIGURE 1 ABOUT HERE

202

203 At the start of each trial, after a brief interval (randomly 1-3 s) an ultra-bright white LED
204 illuminated the single central target ball from the inside. On 60% of the trials for the first 48
205 children, and 50% of trials for the last 251 children, the central ball remained lit, but on the
206 remaining 40% (50%) of trials at the onset of the participant's hand movement the
207 illumination switched from one ball to another in a centre-out configuration. We changed the
208 proportion of trials after the first 48 children in order to have one additional (critical) trial per
209 eccentric ball position. While many researchers present 80% 'unperturbed' and 20%
210 'perturbed' target conditions, this distribution is not universal (e.g., Prablanc and Martin,

211 1992, used 33% unperturbed and 67% perturbed), and neither perturbation probability nor
212 perturbation expectation have strong effects on the latency to initiate movement corrections
213 (Cameron et al., 2013). The hand position was analysed online, and the target change
214 occurred as soon as the tangential velocity of the thumb reached 15 cm/s. This criterion was
215 subsequently changed (after the first 48 children), to a velocity towards the central target of
216 15 cm/s in order to counter the strategy of some children opting to make a short initial
217 movement (e.g., upwards or sideways), before making a second movement towards the
218 target location, which may since have changed. The balls in the up, down, left, and right
219 positions each lit up on 10% (12.5%) of the trials in a pseudorandom order. Children were
220 instructed to start each trial with their thumb and index fingers closed in a pincer grip and
221 placed on the starting point, then to reach and grasp the illuminated ball as accurately and
222 as quickly as possible, but in a controlled manner – as natural a reaching movement as
223 possible. Children were instructed to interrupt their movement to the central ball and grasp
224 instead the eccentric ball when the illumination switched locations. There were 10 practice
225 trials before the main data collection to familiarise the children with the task and this was
226 followed by one testing block of 40 trials. Motion trackers were attached over the thumb and
227 index fingers (i.e., the grasp 'opposition axis', Holt et al., 2013) of a 'NASA' astronaut's glove
228 (this did not appear to affect children's hand movements, see also [Hyde and Wilson, 2011b](#)),
229 to record the position (3 degrees of freedom) of these digits with a Polhemus Fastrack
230 (Polhemus, Colchester, VT, USA) magnetic tracking system. The system has a spatial
231 accuracy of 0.08 cm, and a precision of 0.0055 cm (for the average location sampled in the
232 current study), sampling the two receivers, each at 60 Hz. We opted for two trackers
233 sampling at 60Hz as the ideal trade-off between trackers (1-4) and frequency (120-30Hz) -
234 an additional third tracker on the wrist would have entailed a reduction of sampling frequency
235 to 40Hz. Since human hand and finger movements cannot move or oscillate at much more
236 than 30 Hz (Raethjen et al., 2000), and the visual online control of movement takes a
237 minimum of 100 ms, 60 Hz sampling is more than adequate to capture the relevant
238 information required to test our hypotheses.

239

240 **Cognitive assessments** – Children in the first, MABC-2 (Age band 2, 7-10 years old), group
241 were assessed with the Reading, Verbal Similarities, and Matrices tests of the British Ability
242 Scales (BAS) (Elliot, 1996), and the Conners 3-AI (Conners, 2008). Children in the second,
243 DCDQ'07, group were assessed with the British Picture Vocabulary Scale (Dunn et al.,
244 1997) and the Strengths and Weaknesses of Attention-Deficit/Hyperactivity Disorder
245 Symptoms and Normal Behaviour Scale (SWAN) (Swanson et al., 2001, 2012). Socio-
246 economic status was estimated from children's home postcodes using the UK Government's
247 Indices of Deprivation (IDACI/IMD).

248

249 **Design**

250 All children were assessed with the visual online control test. 187 children were assessed
251 with the MABC-2 (Age band 2, 7-10 years old), and 85 children were assessed with the
252 DCDQ'07. Our study was an exploration to investigate correlations between kinematic
253 variables extracted from reaching and grasping movements, and a) MABC-2 component
254 (manual dexterity, aiming and catching, and balance) and total scores, and b) DDCQ'07
255 scores (coordination; fine motor; general).

256

257 INSERT FIGURE 2 ABOUT HERE

258

259 **Data analysis**

260 The experiments were run and the data analysis was performed using Matlab (Mathworks,
261 Natick, USA), and SPSS for the factor analysis. All the programs and all raw data are or will
262 be freely available from the last author or his website (<http://neurobiography.info/>). All data
263 analysis was fully automated and scripted, using procedures developed during previous
264 work (for full methods and discussion, see Holmes and Dakwar, 2015). A summary of the
265 analytical approach is provided here.

266

267 **Raw data** – Six degree-of-freedom position and orientation data from the index finger and
268 thumb were acquired at 60 Hz for 2 s per trial. Data were re-sampled to 120 Hz then filtered
269 with a 2nd order, zero-lag (dual-pass) Butterworth filter with a 15 Hz low-pass cut-off. Two raw
270 data channels (index finger and thumb), as well as the mean (used for many kinematic
271 parameters), and the difference (used for grip aperture measures), were processed
272 individually by the same analysis script (hl_kinematics.m, part of the HandLabToolBox). The
273 script is fully-automated, and extracts, from each trial, reaction time (RT, the first sample
274 after 100 ms that exceeds 15 cm/s velocity towards the initial target) and movement time
275 (MT, the first sample after RT in which tangential velocity subsequently remains below 10
276 cm/s for at least 50 ms; this is combined with target position information, to check whether
277 MT was reached within, or away from the target location, with a 6 cm tolerance), along with
278 peak acceleration (PA, and the time that PA was reached, TPA), peak velocity (PV, TPV),
279 peak deceleration (PD, TPD), path length, mean velocity (MV), movement symmetry
280 (TPD/MT), movement shape (PV/MV), movement curvature (the maximum deviation
281 orthogonal to the straight line joining the locations at RT and MT, divided by the length of that
282 straight line), and root-mean-squared jerk (3rd differential of position over time) and snap (4th
283 differential). All temporal parameters (TPA, TPV, TPD, MT) are expressed relative to
284 movement onset (i.e., after subtracting RT from the time since the target appeared). The
285 difference between index and thumb positions (i.e., grip aperture) was analysed similarly,
286 yielding measures of peak grip aperture (PGA, TPGA).

287
288 **Processed data** – The analysis routines then processed the data from each trial of each
289 participant, rejected artefacts, determined errors and outliers on a number of criteria.
290 Exclusion criteria were set after an initial analysis, examining the histograms of extracted
291 parameters, and setting limits to exclude only clear outliers during a second analysis. These
292 'outliers' were all caused by participant error (e.g., moving before target onset, or failing to
293 move), or by hardware failure (e.g., the eccentric target light failing to illuminate, magnetic
294 distortion or interruption of the tracker signal). Details of the trials removed are provided in

295 supplementary data. All subsequent calculations were performed on valid trials only, then
296 were summarised per condition (target location) and participant. Where possible, data were
297 extracted from individual trials. Thus, for each participant, condition, and parameter, mean,
298 SD, and N are available. Temporal parameters (TPA, TPV, TPD, TPGA) were also expressed
299 relative to total MT (TPA/MT, TPV/MT, TPD/MT, TPGA/MT). Summary descriptive statistics
300 are provided for all variables in supplementary data. All raw and summary data were
301 inspected visually, in order to set criteria and adjust analytic parameters and procedures.
302 The final analysis is fully-automated and repeatable. The only human intervention in the final
303 analysis was to exclude two clear outlying participants, following plotting of the factor
304 analysis data – factor analysis is sensitive to outliers (Flora et al., 2012).

305

306 **Correction movements** – The principal variables of interest were the latencies, velocities,
307 and accelerations of the corrections made to the reaching component of the movement
308 following target perturbations. By 'correction movements', we mean the velocity of the hand
309 towards the (new, perturbed) target location on trials with a change in target location, minus
310 the same component of velocity on trials without a change in target location. This can be
311 measured in several ways. Following previous work (Holmes and Dakwar, 2015; Oostwoud
312 Wijdenes et al., 2014; Veerman et al., 2008), we used the optimal method (Holmes and
313 Dakwar, 2015) – extrapolating back from the peak correction velocity to the start of the
314 correction velocity curve for each trial (Figure 3). The zero-crossing point on the x-axis is
315 found by extrapolating back from the line joining the 25% and 75% points, relative to the
316 maximum correction velocity (Veerman et al., 2008). This was done both on individual trials
317 as well as on the mean trajectories from trials of the same condition (i.e., right, lower, left, or
318 upper targets), and was implemented by a HandLabToolBox function,
319 `hl_kinematics_correction.m`. To aid comparison with previous similar work, we also
320 calculated the correction time as the 'additional movement time' required (Hyde and Wilson,
321 2011a, 2011b), by subtracting the mean MT on trials without a change in target location from
322 trials with a change.

323

324 To visualise the data, the velocities, accelerations, and jerks across trials in the same
325 condition were averaged by aligning the movement onsets. Each trial was also resampled to
326 120 data points, from RT-5 to MT+5 samples. These resampled, standardised, data were
327 then re-scaled to a maximum height of 1, averaged across conditions per participant, and re-
328 scaled again to a maximum of 1. This re-scaling compensates for between-participant
329 differences in movement velocity, duration, and variability. The final average movement
330 profiles (Figure 4) are then useful to assess the overall 'quality' or 'shape' of movement.

331

332 This analysis revealed a clear progression of velocity and acceleration profiles both as a
333 function of age (Blanchard et al., in preparation), and movement coordination ability (Figure
334 4). Based on this, we also extracted a number of variables in an attempt to measure the
335 overall shape of movement. The area under the velocity curve between RT and MT is
336 equivalent to the path length (i.e., the integral of velocity over time is distance covered), and
337 similar measures can be extracted for the area under velocity, acceleration, and jerk curves,
338 both for the raw, and the resampled standardised data, for both overall 3D velocity, and the
339 component of velocity in the direction of the target change. In our previous work, we found
340 the component of velocity towards the target provided better measures of movement
341 correction (Holmes & Dakwar, 2015). Finally, the additional velocity, acceleration, and jerk on
342 trials with compared to without a change in target location was calculated.

343

344 **Factor analysis** – The typical parameters extracted from position data are highly collinear
345 (Naish et al., 2013). For example, a movement which reaches peak acceleration early will
346 likely also reach peak velocity early; higher acceleration leads to higher velocity; these
347 parameters are correlated. Rather than examine a series of kinematic parameters
348 independently, reducing these highly-correlated variables to a smaller number of more
349 independent factors helps resolve problems with multiple comparisons across different
350 dependent variables. We extracted 87 reaching and grasping parameters from each of 262

351 participants who had valid reaching and grasping data, and reduced this to 17 factors using
352 principal components analysis in SPSS 21 with oblique (direct oblimin) factor rotation in
353 order to minimise the number of variables loading heavily onto each factor. A criterion of
354 eigenvalues >1 was used for factor selection; factor scores were estimated using Bartlett's
355 method. While researchers may disagree over whether and when to use orthogonal or
356 oblique factor rotation, the underlying mathematics is identical, the total variance explained
357 remains the same, and only with criteria external to the factor analysis itself can the
358 usefulness of any particular rotation method be judged (Comrey & Lee, 1992). We assessed
359 the usefulness of the rotation method and the extracted factors by relating their scores to
360 independent measures of movement coordination.

361

362 **Predicting MABC-2 and DCDQ'07 scores with reaching and grasping factors** – The
363 factor scores extracted for each participant and factor were correlated individually with the
364 MABC-2 and DCDQ'07 scores. Further, a stepwise linear regression with all 17 factor scores
365 was run to determine which (if any) of the 17 extracted factors could predict MABC-2 or
366 DCDQ'07 scores.

367

368 Unless otherwise stated, an alpha level of .0125 was adopted. Since both the MABC-2 and
369 DCDQ'07 contain four separate scores, this alpha level corrects for four independent
370 comparisons for each standardised test. Means are reported to 3 significant figures, SDs to
371 the same number of decimal places as the means.

372

373 **Results**

374 A complete table of descriptive summary statistics, along with all the raw data (i.e.,
375 participant means), correlations between variables, and factor analysis results is provided in
376 a supplementary Table, and all the raw data are available freely on request. Here, we
377 summarise only a few pertinent variables. All data are mean±SD unless otherwise stated.

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INSERT FIGURE 3 ABOUT HERE

Reaching and grasping task

Overall, 262 children (age=9.65±0.98 years; 154 females; 20 of whom used their left hand for handwriting) completed the reaching and grasping task with sufficient valid trials (≥20, including at least one successful movement correction) for analysis. Of the 40 trials attempted, 32.7±8.8 valid trials per participant were analysed. Across all participants, 52 trials were excluded for not completing within 2 s; 1259 for reaching and stopping on the central target before making a complete movement correction to the correct target (i.e., corrected 'touchdown' errors); 35 for central touchdowns which were not followed by a complete movement correction; 196 trials for strong magnetic artefacts or other data corruption; 473 for 'outliers' – mostly induced by more subtle magnetic artefacts which were not remedied by initial data filtering. This process led to the removal of 2 participants who no longer had sufficient valid trials for analysis.

Across the valid participants and trials, reaction time (RT) to begin the reaching movement was 364±79 ms (with means ranging between 359 and 371 ms across the five experimental conditions). Movement time (MT) to the central target on unperturbed trials was 514±84 ms; on perturbed trials, movements were completed in means of 731-770 ms. Since a few children did not have valid trials for every target direction, and due to the overall low numbers of perturbed trials, we have not compared movements between the four target locations. There are, however, indications of differences between the left-right and up-down dimensions of movement correction, a finding which will be followed up in a dedicated study.

Using the optimal method from Holmes & Dakwar (2015, Figure 3), the latency to initiate a movement correction following target perturbation was 342±85 ms on average, ranging from 318-335 ms for the right, left, and upper targets, to 390±97 ms for the lower target – this large (≥55 ms) increase in mean latencies for the lower relative to the other targets likely

407 reflects the need to reverse the initial upwards movement required to reach the central
408 target, but this hypothesis needs to be tested with movements starting at the same elevation
409 as the central target. An alternative index of online control measures the additional
410 movement time required to complete the movement correction (MT perturbed minus MT
411 unperturbed, Hyde and Wilson, 2011a). This was 235 ± 90 ms pooled across the four target
412 locations, with right (217 ± 104 ms) and left (214 ± 100 ms) lowest. Unlike for correction
413 latency, additional movement time was greater for the upper (253 ± 101 ms) than the lower
414 (230 ± 103 ms) targets. This difference is discussed below.

415

416 To aid data visualisation, tangential 3D velocity profiles were resampled to 120 points
417 between RT-5 samples and MT+5 samples, then re-scaled to a maximum velocity of 1.
418 Standardised velocity profiles were then averaged across trials, conditions, and participants
419 (Figure 4). Visual inspection of these data prompted additional measures of the area under
420 the velocity, acceleration, and jerk curves to be taken. We expected that the apparent
421 between-participant differences in movement shape on perturbed trials might be important
422 predictors of standardised measures of movement coordination.

423

424 INSERT FIGURE 4 ABOUT HERE

425

426 **Standardised movement measures**

427 Children assessed with the MABC-2 ($n=181$, after removing 6 incomplete datasets) achieved
428 a standard score of 9.19 ± 3.40 ; 25 children were at or below the 5th percentile (i.e., 'possible
429 DCD'), 35 were between the 6th and 16th percentiles inclusive (i.e., 'at risk for DCD', Blank et
430 al., 2012) and 121 were above the 16th percentile. For the DCDQ'07, 85 children's parents
431 rated them as 61.8 ± 17.9 overall. 27 children had total parent ratings below the cut-off for
432 'possible DCD', and 58 above the cut-off.

433

434 **Factor analysis for data reduction**

435 Eighty-seven variables derived from the kinematic data were entered into an exploratory
436 factor analysis with oblique factor rotation. Seventeen resulting factors had eigenvalues >1,
437 accounting for 85.7% of the variance (Table 1). The first three factors had loadings of ≥ 0.3
438 on 50, 40, and 31 original variables respectively, and as such were hard to describe, but
439 likely account for general between-participants' differences in movement speed and
440 variability, or body size, which affects multiple variables. The remaining 14 factors loaded
441 strongly onto between 0 and 18 original variables. An attempt to describe these factors is
442 presented in Table 1, along with the correlation between scores from each factor and the
443 MABC-2 and DCDQ'07 scores. Factors 5, 6, 14, and 15 correlated significantly ($p \leq 0.0125$, 2-
444 tailed) with at least one component of the MABC-2; none correlated significantly with
445 DCDQ'07 scores. The strongest relationship was between factor 6, which explained 4.48%
446 of the reaching and grasping variance, and the MABC-2 aiming and catching component
447 scores ($r_{179} = -.357$, $p < .0001$). Of the original variables, the strongest relationship between
448 kinematic and standard scores was between movement correction latency measured from
449 individual trials (Holmes & Dakwar, 2015) and the aiming and catching score on the MABC-2
450 ($r_{179} = -.260$, $p = .0004$).

451

452 INSERT TABLE 1 ABOUT HERE

453

454 **Predicting MABC-2 and DCDQ'07 scores with reaching and grasping factors**

455 Since the factor rotation method was oblique, the resulting factors could still be collinear,
456 however 17 partially collinear factors are more manageable than 87 more highly collinear
457 original variables. Rather than interpret each of the correlations between factors and MABC-
458 2 scores individually, the 17 factor scores were entered as predictors in a stepwise linear
459 regression to identify those factors which explained significant ($p\text{-enter} \leq 0.0125$, $p\text{-}$
460 $\text{remove} \geq 0.10$) variance in the MABC-2 scores. Only two factors, 6 and 15, were retained in
461 the stepwise regression. Factor 6 was the strongest, and 15 the second predictor of both
462 aiming and catching scores, $F(2, 173) = 17.0$, $p < .0001$, $r^2 = 0.165$, and total MABC-2 scores,

463 F(2, 173)=15.9, $p<.0001$, $r^2=0.155$. Factor 15 was the strongest, and 6 the second, predictor
464 of manual dexterity scores, F(2, 173)=9.48, $p=.0001$, $r^2=0.099$. Finally, factor 15 was the sole
465 predictor of balance scores, F(1, 174)=7.17, $p=.008$, $r^2=0.040$. The regression coefficients
466 are provided in Table 1, and the whole model fits in Figure 5.

467

468 The factor analysis and subsequent stepwise regression identified factors 6 and 15 as clear
469 and strong predictors of MABC-2 scores, particularly for the aiming and catching component.
470 Factor 6 loaded most strongly ($\geq.3$) on the additional area under the jerk and acceleration
471 curves in perturbed compared to unperturbed trials, expressed either as a difference (jerk:
472 .512, acceleration: .321) or a ratio (.479, .314), the SD of TPGA (.491), the relative time of
473 peak acceleration (-.420), path length mean (.407) and SD (.354), the SD of MT (.393), the
474 standardised area under the jerk curve (-.372), the mean correction latency per trial (.322),
475 mean curvature (.308), and the SD of jerk (-.302). Since factor 6 was negatively correlated
476 with the MABC-2 scores, larger increases in jerk and acceleration and later corrections on
477 perturbation trials, longer and more curved paths, higher variability of grip timing, MT, and
478 path, along with relatively earlier peak acceleration, and lower jerk predicted lower MABC-2
479 scores. Factor 15 loaded strongly ($\geq.3$) on the SD of PGA (.380), the relative time of PGA
480 (.377), and the standardised area under the jerk curve (.310). Since factor 15 was positively
481 correlated with the MABC-2, more variable and relatively later peak grip aperture and larger
482 areas under the standardised jerk curves predicted higher MABC-2 scores.

483

484 INSERT FIGURE 5 ABOUT HERE

485

486 **Group analyses**

487 The relationships between reaching and grasping and standardised movement coordination
488 scores seem to be continuous, rather than containing any discontinuities at particular scores
489 or ranges. Nevertheless, following a reviewer's request, the continuum was divided into
490 discrete groups on the basis of both clinical diagnoses (e.g., DCD diagnosis) and the MABC-

491 2 and DCDQ'07 scores relating to clinically significant cut-offs. In our sample, 11 children
492 had formal diagnoses of DCD; 25 children (13.8% of our sample) were at or below the 5th
493 percentile of the MABC-2; 35 (19.3%) were between the 6th and 16th percentile inclusive; and
494 121 (66.8%) had scores above the 16th percentile. For the DCDQ'07, a large proportion
495 (31.7%) of parents rated their children as having movement coordination below the cut-off.
496 These groups were compared on factors 6 and 15 from the factor analysis, and on the model
497 prediction scores (summary data in the supplementary table).

498
499 Children at or below the 5th percentile on the MABC-2 had significantly different ($p \leq .025$, 1-
500 tailed, correcting for 2 comparisons) scores from children above the 16th percentile on both
501 factors 6, $t_{139} = 3.08$, $p = .001$, and 15, $t_{139} = -2.37$, $p = .01$, and children between the 6th and 16th
502 percentiles inclusive also differed from the >16th percentile group on factor 6 ($t_{151} = 2.19$,
503 $p = .015$), but not factor 15, $t_{151} = -1.25$, $p = .11$. Factor scores of the groups at or below the 5th
504 and between the 6th and 16th inclusive did not differ significantly. Regarding the linear model
505 predictions of the MABC-2 component scores and total scores, the same pattern was found,
506 with the two lower-scoring MABC-2 groups differing significantly ($p \leq .0125$, 1-tailed,
507 correcting for 4 comparisons) from the higher-scoring group on manual dexterity, aiming and
508 catching, and total scores, while only the comparison between the $\leq 5^{\text{th}}$ percentile group and
509 the >16th percentile group was significant for the balance scores. All the differences were in
510 the expected directions, which is not surprising as the models were set up to predict these
511 scores – dividing the range into bins and re-testing is a statistical 'double-dip'. There was no
512 evidence for significant differences between the 11 children with a formal diagnosis of DCD
513 and the rest of the sample, either on factor 6, $t_{255} = 0.663$, $p = .51$ or factor 15, $t_{255} = -1.26$,
514 $p = .21$, or on the aiming and catching, balance, or total scores ($|t_{174}|s < 1.68$, $ps > .095$). Again,
515 this may not be surprising, as the model was set up to predict MABC-2 scores, rather than
516 DCD diagnosis. Factor 12, however, did show a relatively large difference between children
517 with DCD and those without, $t_{255} = -2.72$, $p = .007$ – the 11 children with DCD had larger, earlier

518 peak grip apertures, and made more additional acceleration on perturbed trials, as
519 compared to children without DCD.

520

521 By contrast to the MABC-2, children with low versus high parent ratings of movement
522 coordination (DCDQ'07) did not differ significantly in their factor scores, although the
523 direction of effects was equivalent to those in the MABC-2 groups. Finally, while responding
524 to reviewers' comments, we discovered several significant differences in the factor scores for
525 participants who performed the task in the dark versus in the light, who used their dominant
526 versus their non-dominant hand to reach, and based on their gender. Analysis of these
527 categorical variables, along with age and other participant-specific predictors, is beyond the
528 current scope and will be dealt with fully elsewhere (Blanchard et al., in preparation).

529

530 **Discussion**

531 The aim of this study was to investigate which kinematic variables of the visual online control
532 of reaching and grasping movements could predict the standard scores of MABC-2 and
533 DCDQ'07. Our results show that two factors extracted from a large number of movement
534 variables provided strong predictions of MABC-2 performance, most strongly for aiming and
535 catching scores. None of the factors individually or combined significantly predicted the
536 DCDQ'07 scores. In the following, we discuss the relationships between reaching and
537 grasping and the MABC-2, focussing on the measurement and analysis of movements in
538 double-step perturbation tasks.

539

540 **Sensorimotor processes underlying reaching, grasping, catching, and aiming**

541 Performance of our reaching and grasping task requires accurate planning, generation, and
542 visual online control of reach-to-grasp movements, including the coordination of reaching
543 and grasping phases. From our results, the strongest predictor of MABC-2 scores (especially
544 the aiming and catching component) was factor 6, which loaded heavily on measures of the
545 additional acceleration and jerk on perturbed compared to unperturbed trials, movement

546 path, curvature, the latency to initiate movement corrections, and peak grip aperture. This
547 factor may represent the key sensorimotor processes required in visual online control.
548 Following a change in target location, the ideal movement correction would comprise a
549 change of direction towards the new target, but without an overall increase in movement
550 speed (i.e., no additional acceleration or jerk), and with a minimum overall increase in
551 movement path length and duration. Efficient corrections will thus have lower overall jerk,
552 path, movement time, curvature, and correction latency. Factors 6 and 15 also loaded on the
553 variability and relative timing of peak grip aperture. An ideal correction to the reaching
554 component of the movement should not also require a correction to the grasping component.
555 Children who correct their reaching movement optimally would not need to adjust their
556 grasping movement - the time to peak grasp aperture could stay relatively constant relative
557 to overall movement time. By contrast, children who fail to adjust their reaching movement
558 efficiently might close their grasp onto the central target, then require an additional opening
559 of the grasp for the peripheral target. On some trials, the initial grasp will be detected as the
560 peak grip aperture, and on other trials peak aperture will occur on the second grasp. This
561 double-grasping movement leads to greater variability in the measured relative time of peak
562 grip aperture. Our result echoes an earlier finding in which children with DCD showed a
563 much greater variability in grasp timing than typically developing children (Astill and Utley,
564 2008). The authors of this previous study suggested that children with coordination disorders
565 may use a decomposition strategy to simplify the control of transport and grasp phases of
566 catching by uncoupling these movement components.

567

568 While aiming and catching scores were best-predicted by the reaching and grasping factors
569 (16% of variance in the MABC-2 explained), manual dexterity, and to a lesser extent balance
570 scores, were also significantly predicted by reaching and grasping, with 10% and 4% of
571 variance explained, respectively. Because scores across the three components of the
572 MABC-2 are correlated (across 225 of our participants, manual dexterity component scores
573 correlate with aiming and catching, $r_{223}=.342$, and balance, $r_{223}=.525$; aiming and catching

574 correlates with balance, $r_{225}=.389$), factors which predict one of the components are also
575 likely to predict the others. This is likely due to general movement coordination ability, to
576 general cognitive, attentional, or motivational factors which are common to the movement
577 tasks, or to the fact that accurate control of the hands and arms also requires postural and
578 balance control, leading to functional links in development of these abilities (Flatters et al.,
579 2014).

580

581 The relationship between kinematic factors and the aiming and catching component of the
582 MABC-2 (16% variance explained) was modest, given that, for example, the manual
583 dexterity and balance components shared 28% of variance in our dataset. Nevertheless, we
584 found no significant relationships at all between any of our kinematic factors and the
585 DCDQ'07 parent questionnaire. This negative finding suggests that parents' evaluations of
586 how their child's movement coordination ability compares with others' should be interpreted
587 cautiously. The DCDQ'07 alone may be unlikely to measure movement coordination skill, at
588 least for reaching, grasping, aiming, and catching skills, although note that we did not
589 measure the DCDQ'07 and the MABC-2 in the same children.

590

591 Finally, no significant relationship was found between reaction time variables or the factors
592 that loaded heavily on them, and the MABC-2 scores. Henderson and colleagues (1992)
593 observed both prolonged simple reaction time and movement time in simple aiming in
594 children with DCD. However, Hyde and Wilson, (2013) found that RT in children with mild to
595 moderate motor impairments (DCD) was not significantly different than in TD children. The
596 authors used this result as evidence to support the claim that there is not a basic information
597 processing impairment in children with DCD. However, earlier work (Henderson et al., 1992;
598 Hyde and Wilson, 2011a, 2011b) found longer RT to targets in children with motor
599 impairment compared to matched controls, and is also consistent with other literature
600 showing longer RT to external stimuli in children with DCD under lighting conditions which
601 did not permit children to see their moving limb (Wilson and Hyde, 2013; Wilson and

602 McKenzie, 1998). It is likely, then, that differences in RT between groups of children with and
603 without DCD or other motor disorders are task-dependent (Mon-Williams et al., 2005).

604

605 **Measuring rapid visual online control**

606 One important aspect of the present work concerns the method of measuring online
607 movement corrections. Many different methods are possible and useful in different contexts
608 (Holmes and Dakwar, 2015; Oostwoud Wijdenes et al., 2014), but the optimal methods in the
609 present context involve fitting a model to the expected velocity or acceleration curves that
610 arise from correction movements (Veerman et al., 2008). Previous studies have used
611 manual estimation of trajectory deviations (e.g., Hyde and Wilson, 2011b, 2013), but these
612 methods are time-consuming and prone to experimenter bias or error. Our fully-automated
613 analysis extracted a number of variables reflecting the latency, velocity, and acceleration of
614 movement corrections, and performed this analysis on both individual trials and the
615 averaged velocities across trials. We found important discrepancies between methods of
616 measuring online control: First, using average movement trajectories can result in
617 substantially shorter correction latencies than using individual trial-by-trial analyses, due to
618 temporal smoothing and broadening of velocity curves. The mean correction latency based
619 on individual trials was 342 ms, while the mean based on the means of trials was 299 ms.
620 Second, correction latencies based on differences in total movement time, which confounds
621 correction latency with the post-correction movement time, were just 235 ms, more than 100
622 ms less than that of the individual trial-by-trial analysis. The additional movement time
623 following a movement correction will be lower in children who reach faster or straighter
624 overall, or who execute a faster correction movement. Indeed, the 107 ms difference
625 between our preferred measure of correction latency and the additional movement time
626 suggests that children increase their movement speed substantially after the target change,
627 'catching-up'. While our preferred correction latency measure was longest for the lower
628 target location, the additional movement time required was longest for the upper target
629 location. Moving the arm upwards probably requires more effort than moving downwards, so

630 the post-correction movement direction may well influence overall movement time.
631 Correction latencies from different studies can only meaningfully be compared if identical
632 methods were used to measure them.

633
634 We chose to extract as many variables as possible from the reaching and grasping
635 movements in an attempt to fully capture the differences in movement between children and
636 conditions. With 87 extracted variables, the problem of multiple comparisons and collinearity
637 arises, which we addressed by reducing the data to 17 relatively independent factors (cf
638 Naish et al., 2013). An alternative, preferable, but computationally-expensive approach is to
639 fit a series of low-dimensional models to the raw velocity data, and to analyse only the model
640 parameters across participants and conditions. This analysis of 'sub-movements' is based on
641 the minimum-jerk model, and may account well for online movement corrections (Flash and
642 Henis, 1991). This approach, using constrained non-linear optimisation in Matlab, was
643 investigated for analysis of the current dataset. However, with 262 participants and 40 trials,
644 the computer processor time alone was likely to take several months! We will use this
645 technique for future work.

646

647 **Continuous versus discrete groups of movement ability**

648 Our approach to data analysis was continuous, in that we did not set out to create two
649 distinct groups consisting of children with DCD and TD children. Rather, we explored motor
650 abilities across the spectrum, eliminating the difficulties that arise when trying to categorise
651 DCD, which is well known for its heterogeneity (Zwicker et al., 2012). We have noted that
652 diagnosis of DCD is incomplete in the local population, and variable between groups of
653 children, for example from different schools or administrative areas. Furthermore, we found
654 that some children with a diagnosis of DCD performed perfectly well on the MABC-2. This
655 could be due either to the wrong diagnosis being made, an intervention having been
656 effective, developmental improvements since diagnosis, or to the inadequacy of the MABC-2
657 as a diagnostic instrument (Venetsanou et al., 2011). In the absence of a diagnosis, then,

658 any division of continuous MABC-2 data into discrete clinical (i.e., $\leq 5^{\text{th}}$ percentile) or pre-
659 clinical (i.e. $6^{\text{th}} < \text{percentile} \leq 16^{\text{th}}$) categories is arbitrary, and, we suggest, likely to obscure
660 the underlying, probably continuous, relationships between individual movement parameters
661 and performance on the MABC-2. We have also noted that ceiling effects and the non-
662 parametric distribution of data in some MABC-2 tasks limits the sensitivity of the MABC-2 to
663 measure the full, continuous range of movement skill, and may have substantial implications
664 for interpreting the standard cut-offs at the 5^{th} and 16^{th} percentiles (French et al., in
665 preparation).

666

667 **Conclusions**

668 Our results support the interpretation that impaired visual online control is a strong predictor
669 of performance on standard tests of movement ability, as are often used to diagnose
670 developmental movement disorders. The visual online control task developed for this study
671 provides a continuous and high-resolution measurement, and is directly comparable
672 between adults and children, which makes it a promising task for further study. The present
673 results show that children who are poor at aiming and catching are also particularly poor at
674 the online control of reaching and grasping.

675 **Conflict of Interest Statement**

676 The authors declare that the research was conducted in the absence of any commercial or
677 financial relationships that could be construed as a potential conflict of interest.

678

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682

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826 **Figure legends**

827

828 Figure 1: Experimental apparatus. Children sat and rested their hand on a table, keeping
829 their index finger and fingers in a 'start' location (black hemisphere), 30cm away from a
830 vertical board with five orange table tennis balls attached at the centre, top, bottom, right and
831 left sides - the centres of the four eccentric balls were 11.5cm away from the centre. Children
832 wore a glove with trackers (solid grey circles) attached on the index finger and thumb.

833

834 Figure 2: Recruitment and selection. 299 participants were recruited through schools,
835 parents, a DCD support group and a University public engagement event. After removing
836 outliers and artefacts, 262 datasets entered the factor analysis. 181 valid datasets with
837 MABC-2 scores, and 85 valid datasets with DCDQ'07 scores were available for regression
838 analysis. FA: Factor analysis; MABC-2: Movement Assessment Battery for Children-2;
839 DCDQ'07: Developmental Coordination Disorder Questionnaire'07.

840

841 Figure 3: Automated data analysis. Two typical trials, taken from participant number 1,
842 illustrating the automated analysis. Data have been re-aligned to movement onset. **A.** Raw
843 x, y, and z position data from an unperturbed trial. **B.** 3D velocity from the same unperturbed
844 trial indicated in A. RT: Reaction time; PA: Peak acceleration; PV: Peak velocity; PD: Peak
845 deceleration; MT: Movement time. **C.** 3D velocity from a perturbed trial. Note the additional
846 velocity curve, starting at about 0.3 s. **D.** 3D correction velocity: the difference in velocity
847 between the perturbed and an unperturbed trial (for illustration only; the mean unperturbed
848 velocity per participant was used in the analysis). CT: Correction time, determined by
849 extrapolating the line joining the 25% and 75% points on the correction velocity curve
850 (circles), back to the x-axis (Holmes & Dakwar, 2015; Veerman et al., 2008); CT-slope: the
851 slope of the line joining the 25% and 75% lines; CT-mag: the peak correction velocity. **E.**
852 Grip aperture from the same trial as illustrated in C-D. PGA: Peak grip aperture.

853

854 Figure 4: Mean velocity profiles highlight substantial differences in online control as a
855 function of total MABC-2 score. The central panel shows normalised velocity profiles on trials
856 with unperturbed targets, for three groups of children separated according to their overall
857 MABC-2 score: $\leq 5^{\text{th}}$ percentile (black); $> 5^{\text{th}}$ and $\leq 16^{\text{th}}$ percentile (mid-grey); $> 16^{\text{th}}$ percentile
858 (light grey). The four other panels show velocity profiles for the same three groups in the four
859 conditions with perturbations of target location. For all perturbed targets, the second velocity
860 peak (at around 70-80 samples) is more smoothly integrated with the first in children with
861 higher MABC-2 scores. Children with the lowest scores on the MABC-2 show the largest
862 changes in velocity between the first and second velocity peaks. The broken black lines
863 show the SE for the $\leq 5^{\text{th}}$ percentile group. The other groups had similar error bars and are
864 not shown for clarity.

865
866 Figure 5: Reaching and grasping factors predict MABC-2 performance. Linear models
867 combining factors 6 and 15 from the factor analysis explain a significant proportion of
868 variance (r^2) in children's MABC-2 performance (y-axes, MABC-2 component and total
869 scores). X-axes show standardised model predictions. The trend line shows the model fit,
870 with 95% confidence intervals. Reaching and grasping explains 17% of the variance in
871 aiming and catching scores, 16% of variance in the total scores, 10% of the manual
872 dexterity, and 4% of the balance score variance.

Table 1: Factors extracted from 87 kinematic variables, and their relationship with MABC-2 and DCDQ-07 scores

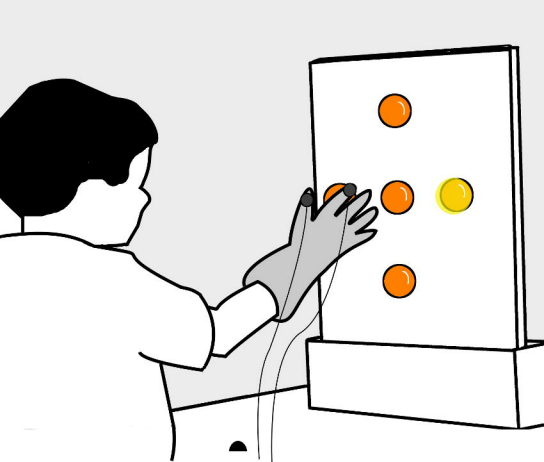
Factor	Loadings ≥±0.3 (N)	Description†	Variance explained (%)	Correlation with MABC-2 component scores, r_{185} (stepwise regression coefficient±SE)				Correlation with DCDQ-07 scores, r_{83}			
				MD	A&C	B	T	C	F	G	T
1	50	-	25.4	.050	.020	.051	.054	.019	.111	.069	.069
2	40	-	13.0	-.040	.010	-.016	-.023	-.127	-.068	-.068	-.106
3	31	-	10.3	.022	-.067	-.007	-.014	-.086	-.024	-.048	-.066
4	18	'Temporal variability; slow corrections'	6.48	.050	.134	.111	.118	-.068	.118	.032	.016
5	18	-	5.24	-.186*	-.140	-.183*	-.217*	-.202	-.016	.011	-.093
6	14	'Jerk, path, correction latency, curvature'	4.48	-.210*	-.357*	-.182*	-.294*	-.079	-.123	-.051	-.093
				(-1.55±0.537)	(-1.77±0.344)		(-4.77±1.14)				
7	8	'Additional movement during corrections'	2.99	.031	-.139	.169	.055	.223	.110	.130	.187
8	3	'Early peak grip aperture'	2.51	.000	-.064	-.034	-.036	.067	-.090	.038	.020
9	5	'High correction magnitude variability; long paths'	2.45	.089	.060	.032	.074	-.194	-.038	-.143	-.158

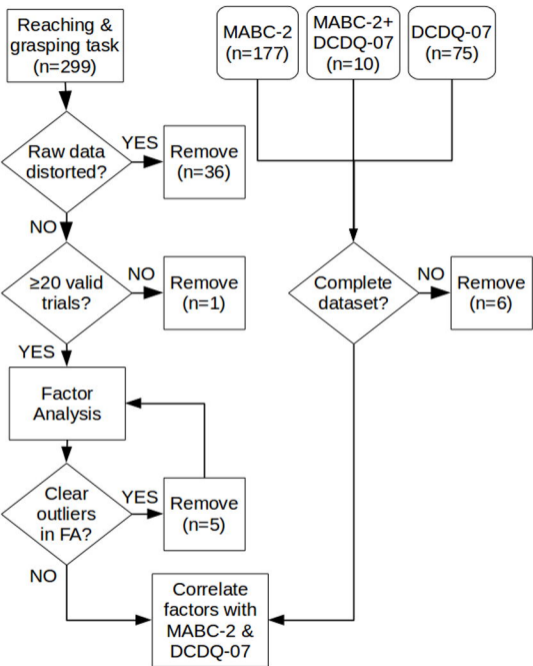
10	4	'Additional acceleration/jerk; correction variability	2.12	.020	-.031	.027	.013	.037	.085	-.050	.022
11	5	'Low correction magnitude and grip timing variability'	2.06	.129	.177	.103	.163	.038	-.146	.002	-.024
12	4	'Smaller, later peak grip aperture'	1.76	.044	.032	.091	.074	.034	.132	.122	.103
13	5	'Slow RT; long correction paths'	1.66	-.047	.036	.129	.053	-.122	-.057	-.131	-.125
14	0	('Path variability')	1.53	.213*	.136	.148	.211*	-.036	-.001	-.049	-.037
15	3	'Variable and late peak grip aperture'	1.32	.235*	.194*	.199*	.264*	.196	.231	.215	.244
				(1.68±0.517)	(0.918±0.332)	(1.54±0.573)	(4.12±1.10)				
16	2	'Long reaction time'	1.29	-.134	-.092	-.082	-.129	-.092	-.148	-.054	-.107
17	2	'Variable peak grip aperture; straight reaches'	1.16	-.001	-.164	-.083	-.091	-.091	-.130	-.118	-.127

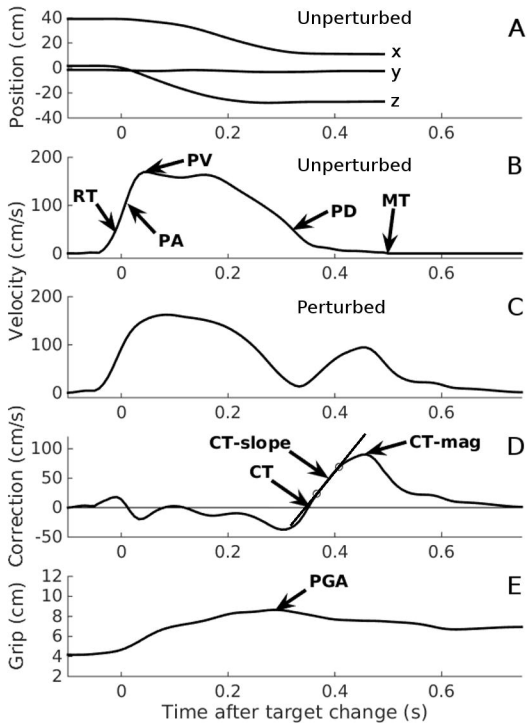
874 † Descriptions are subjective and approximate; a full list of factor coefficients is provided in the Supplementary Tables. MD: Manual dexterity;

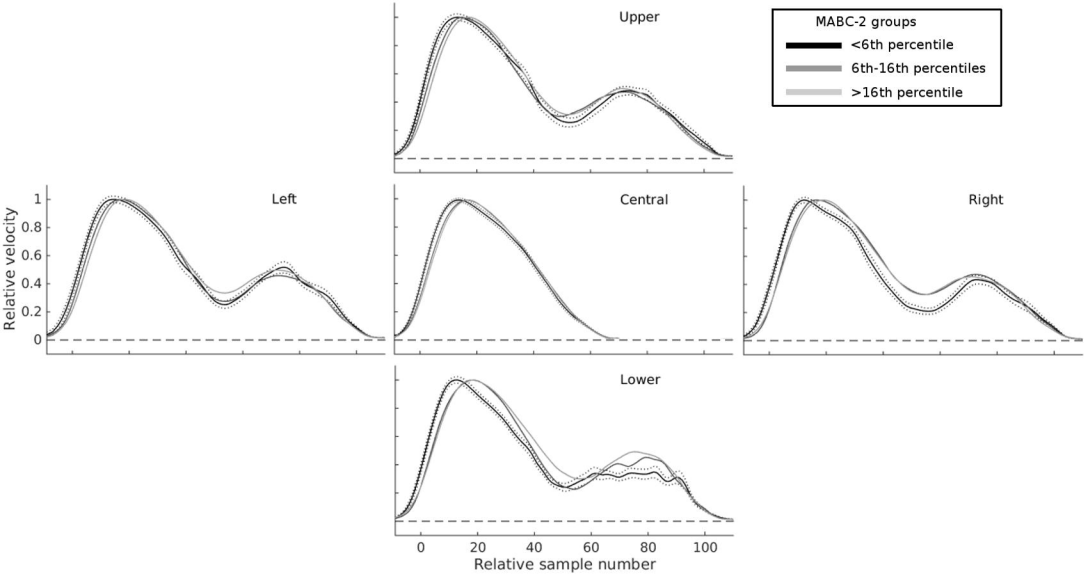
875 A&C: Aiming and catching; B: Balance; T: Total; C: Coordination during movement; F: Fine motor; G: General. *p≤.0125 (corrected for 4

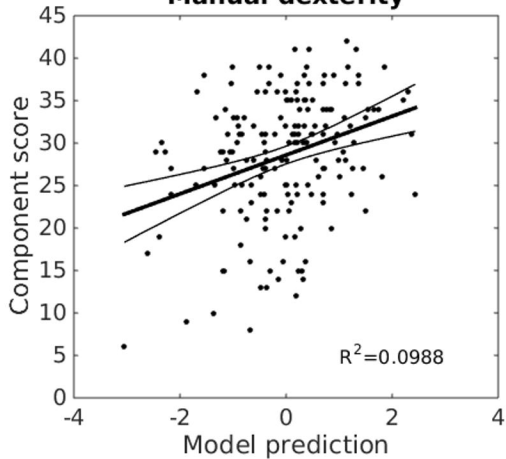
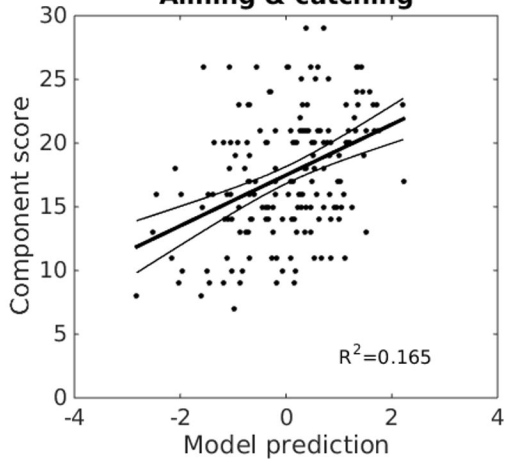
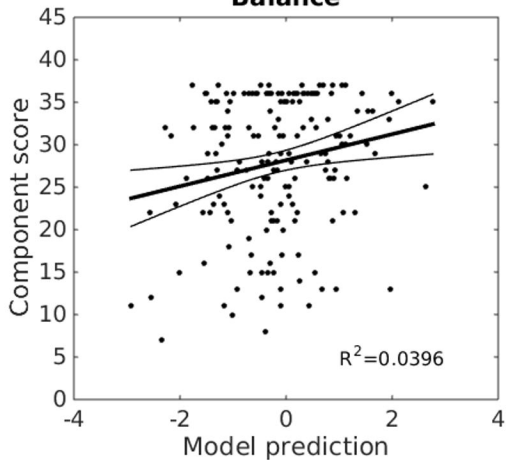
876 comparisons per factor). Values in parentheses are the coefficients \pm standard errors of the factors that remained as significant predictors in a
877 stepwise linear regression ($p < .0125$).









Manual dexterity**Aiming & catching****Balance****Total**