

1 **Activity in the Fronto-Parietal Multiple-Demand Network is Robustly**
2 **Associated with Individual Differences in Working Memory and Fluid**
3 **Intelligence**

4

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19

20 **Abstract**

21 Numerous brain lesion and fMRI studies have linked individual differences in executive
22 abilities and fluid intelligence to brain regions of the fronto-parietal “multiple-demand”
23 (MD) network. Yet, fMRI studies have yielded conflicting evidence as to whether better
24 executive abilities are associated with stronger or weaker MD activations and whether
25 this relationship is restricted to the MD network. Here, in a large-sample (n=216) fMRI
26 investigation, we found that stronger activity in MD regions – functionally defined in
27 individual participants – was robustly associated with more accurate and faster
28 responses on a spatial working memory task performed in the scanner, as well as fluid
29 intelligence measured independently (n=114). In line with some prior claims about a
30 relationship between language and fluid intelligence, we also found a weak association
31 between activity in the brain regions of the left fronto-temporal language network during
32 an independent passive reading task, and performance on the working memory task.
33 However, controlling for the level of MD activity abolished this relationship, whereas the
34 MD activity-behavior association remained highly reliable after controlling for the level of
35 activity in the language network. Finally, we demonstrate how unreliable MD activity
36 measures, coupled with small sample sizes, could falsely lead to the opposite, negative,
37 association that has been reported in some prior studies. Taken together, these results
38 demonstrate that a core component of individual differences variance in executive
39 abilities and fluid intelligence is selectively and robustly positively associated with the
40 level of activity in the MD network, a result that aligns well with lesion studies.

41

42 **Keywords**

43 Fronto-parietal; executive functions; fluid intelligence; individual differences; multiple-

44 demand; language

45

46 **Introduction**

47 General cognitive abilities, such as fluid intelligence, and the tightly linked executive
48 abilities, are among the best predictors of academic achievement and professional
49 success (Gottfredson, 2002; Kuncel & Hezlett, 2010; Plomin & Deary, 2015). These
50 abilities are thought to rely on a network of bilateral frontal and parietal brain regions.
51 Selective damage to these regions is associated with disorganized executive behavior
52 and significant loss of fluid intelligence (Duncan, Burgess, & Emslie, 1995; Glascher et
53 al., 2010; Roca et al., 2010; Warren et al., 2014; Woolgar, Duncan, Manes, &
54 Fedorenko, 2018; Woolgar et al., 2010). Similar frontal and parietal regions are
55 activated in brain imaging studies during diverse demanding tasks, including
56 manipulations of working memory, fluid reasoning, selective attention, set shifting,
57 response inhibition, and novel problem solving inter alia (Assem, Glasser, Essen, &
58 Duncan, 2020; Michael W. Cole & Schneider, 2007; Dosenbach et al., 2006; Duncan,
59 2000, 2010; Duncan & Owen, 2000; Fedorenko, Duncan, & Kanwisher, 2013; Geake &
60 Hansen, 2005; Vakhtin, Ryman, Flores, & Jung, 2014). We refer to this set of brain
61 regions as the “multiple-demand” (MD) network (following Duncan, 2013, 2010) given
62 their sensitivity to multiple task demands. The MD network includes lateral and
63 dorsomedial frontal areas, anterior insular areas, and areas along the intra-parietal
64 sulcus (Assem et al., 2020; Fedorenko et al., 2013), and these areas form a functionally
65 integrated system as evidenced by strong synchronization during naturalistic cognition
66 (Assem et al., 2020; Blank, Kanwisher, & Fedorenko, 2014; Paunov, Blank, &
67 Fedorenko, 2019).

68 Prior fMRI studies have linked activity in the MD network with individual
69 differences in executive abilities and fluid intelligence, but have left open the nature of
70 this relationship. First, conflicting claims have been made regarding the direction of
71 brain-behavior correlations across individuals. On the one hand, some have found that
72 stronger MD activation is associated with worse performance on executive tasks and
73 lower IQ (Basten, Hilger, & Fiebach, 2015; Deary, Penke, & Johnson, 2010; Dunst et
74 al., 2014; Haier et al., 1988; Neubauer & Fink, 2009; Rypma et al., 2006; Rypma &
75 Esposito, 2000; Santarnecchi, Galli, Polizzotto, Rossi, & Rossi, 2014; Stern, Gazes,
76 Razlighi, Steffener, & Habeck, 2018). Such studies have typically advocated a “neural
77 efficiency” explanation: smarter individuals can use fewer neural resources to achieve
78 the same level of performance. On the other hand, others have found the opposite
79 pattern, where stronger MD activation is associated with better executive task
80 performance and higher IQ (Basten, Stelzel, & Fiebach, 2013; Burgess, Gray, Conway,
81 & Braver, 2011; Choi et al., 2008; M. W. Cole, Yarkoni, Repovs, Anticevic, & Braver,
82 2012; Gray, Chabris, & Braver, 2003; Lee et al., 2006; Tschentscher, Mitchell, &
83 Duncan, 2017). In an attempt to reconcile these conflicting findings, some have
84 suggested that the direction of the correlation may depend on task difficulty with “neural
85 efficiency” (i.e., a negative association between MD activity and performance) observed
86 in easier tasks, and positive associations observed during more complex tasks
87 (Neubauer & Fink, 2009; Sripada, Angstadt, Rutherford, Taxali, & Shedden, 2020).

88 Relatedly, superior executive abilities and higher IQ have been reported to
89 correlate with stronger synchronization (typically, estimated during rest e.g. Fox et al.,
90 2005) among the MD brain regions (M. W. Cole et al., 2012; Dubois, Galdi, Paul, &

91 Adolphs, 2018; Ferguson, Anderson, & Spreng, 2017; Finn et al., 2015; Hearne,
92 Mattingley, & Cocchi, 2016; Smith et al., 2015), although most of these studies have
93 relied on the same resting-state Human Connectome Project (HCP) dataset (Smith et
94 al., 2013). Fewer studies have reported weaker synchronization in such individuals
95 (Santarnecchi et al., 2014; van den Heuvel, Stam, Kahn, & Hulshoff Pol, 2009).

96 A second open question concerns the specificity of this relationship to the MD
97 network. Challenging the idea that executive functions are selectively tied to this
98 network, a number of fMRI studies have also linked individual differences in executive
99 abilities and fluid intelligence with activity in other brain regions/networks, including
100 occipito-temporal areas (Haier, White, & Alkire, 2003; Park, Carp, Hebrank, Park, &
101 Polk, 2010) but see (Assem et al., 2020; Sani, McPherson, Stemmann, Pestilli, &
102 Freiwald, 2019) for evidence that these regions may belong to an extended MD
103 network), the default mode network (DMN) (Lipp et al., 2012; Smith et al., 2015), or the
104 degree of MD-DMN differentiation (Sripada et al., 2020). A recent study used 7 fMRI
105 tasks from the HCP dataset to demonstrate that task activation levels in many brain
106 regions can, to some extent, predict individual differences in general intelligence,
107 though critically, MD regions—engaged by executive function tasks—are the best
108 predictors (Sripada et al., 2020). In contrast, another recent study using the HCP
109 resting-state dataset showed that the strength of inter-region correlations in most brain
110 networks predicts general intelligence, and to a similar extent (Dubois et al., 2018). A
111 key potential limitation of these studies is that, like the above-mentioned studies, they
112 rely exclusively on the HCP dataset and are yet to be replicated in independent data.

113 These apparently discrepant results could reflect the complexity of the brain-
114 behavior relationship in the domain of executive abilities, with perhaps multiple
115 underlying cognitive constructs (Miyake & Friedman, 2012) and neural mechanisms
116 contributing to their implementation. However, a number of methodological limitations
117 plague previous studies and may, instead, explain away some of these discrepancies.
118 *First*, many earlier studies have used small numbers of participants (as low as n=8)
119 and/or transformed continuous behavioral measures into categorical variables (e.g.,
120 high- vs. low-performing participants). Both of these factors can produce inflated or
121 spurious relationships (Haier et al., 1988; Lee et al., 2006; Rypma et al., 2006; Rypma &
122 Esposito, 2000; Wager et al., 2005). *Second*, most studies have failed to assess the
123 reliability of the relevant behavioral and/or brain measures (e.g., the strength of the
124 BOLD response, or the strength of inter-regional synchronization) – a critical
125 prerequisite for relating behavioral and brain individual variability (Dubois & Adolphs,
126 2016). Both behavioral and brain measures have to be stable within individuals over
127 time (e.g., across multiple runs of a task, or across tasks) (Mahowald & Fedorenko,
128 2016). This is especially important for studies using BOLD estimates based on contrasts
129 of task relative to fixation, or resting-state inter-region synchronization measures, which
130 may fail to isolate MD activity from general state variables, like motivation, arousal, or
131 caffeine intake (Basten et al., 2013; M. W. Cole et al., 2012; Dubois et al., 2018; Dunst
132 et al., 2014; Gray et al., 2003; Rypma et al., 2006; Rypma & Esposito, 2000; Smith et
133 al., 2015; Stern et al., 2018; Wager et al., 2005). *Third*, almost all previously mentioned
134 studies have failed to take into consideration individual variability in the precise
135 locations of the MD regions (see (Assem et al., 2020; Blank, 2020; Fedorenko et al.,

136 2013; Shashidhara, Spronkers, & Erez, 2020) for evidence of such variability). This
137 variability leads to losses in sensitivity and functional resolution (Brett, Johnsrude, &
138 Owen, 2002; Nieto-Castañón & Fedorenko, 2012; Saxe, Brett, & Kanwisher, 2006), and
139 it also affects the interpretation of inter-regional functional synchronization findings
140 (Bijsterbosch, Beckmann, Woolrich, Smith, & Harrison, 2019; Bijsterbosch et al., 2018).
141 This problem is compounded by the proximity of MD areas to functionally distinct areas
142 such as language-selective regions (Fedorenko, Duncan, & Kanwisher, 2012), which
143 show no response to any demanding task other than language processing (Fedorenko,
144 Behr, & Kanwisher, 2011; Fedorenko & Blank, 2020; Fedorenko & Varley, 2016; Monti,
145 Parsons, & Osherson, 2012). And *fourth*, many studies have failed to adequately
146 assess the selectivity of the relationship between MD activity and behavior (Choi et al.,
147 2008; M. W. Cole et al., 2012; Dubois & Adolphs, 2016; Gray et al., 2003; Rypma et al.,
148 2006). This is important given that trait variables (e.g., brain vascularization) are known
149 to affect neural responses (e.g., Ainslie and Duffin, 2009; Kazan et al., 2016), so in
150 order to argue that the MD network's activity relates to individual differences in
151 executive functions or fluid intelligence, it is important to demonstrate that activity in
152 some other, control, brain region or network does not show a similar relationship.

153 To circumvent these limitations and rigorously test the relationship between MD
154 activity and executive abilities and fluid intelligence, we conducted a large-scale fMRI
155 study, where participants (n=216) performed a spatial working memory (WM) task that
156 included a harder and an easier condition. We first established the reliability of the
157 Hard>Easy (H>E) BOLD effect in the MD network (defined functionally in each
158 participant individually (Fedorenko et al., 2013)), and then examined the relationship

159 between the size of this effect and a) behavioral performance on the task (including in
160 an independent run of data), and b) fluid intelligence (in a subset of participants, n=114).
161 We further evaluated the selectivity of this MD-behavior relationship by examining fMRI
162 responses in the left fronto-temporal language network while the same participants
163 performed a language comprehension task (Fedorenko et al., 2010). This network
164 serves as a good control because, on the one hand, the language network is robustly
165 functionally distinct from the MD network (Blank et al., 2014; Diachek, Blank,
166 Siegelman, Affourtit, & Fedorenko, 2020; Fedorenko & Blank, 2020; Mineroff, Blank,
167 Mahowald, & Fedorenko, 2018), but on the other hand, language has long been
168 implicated in abstract and flexible thought (e.g., Bickerton, 1995; Carruthers, 2002;
169 Dennett, 1997; cf. Fedorenko and Varley, 2016), including some studies that have
170 linked damage to the regions of this network to performance on some fluid reasoning
171 tasks (e.g., Baldo et al., 2010; cf. Woolgar et al., 2018).

172 To foreshadow our results, we found that stronger (rather than weaker) MD
173 responses were associated with better performance on the spatial WM task as well as
174 higher fluid intelligence scores. The strength of activity in another large-scale network –
175 the language network – did not explain any additional variability in WM task
176 performance (i.e., it showed a weak correlation with behavior, which was eliminated
177 once the level of MD activity was taken into account). Finally, we demonstrate how
178 unreliable MD activity measures, coupled with small sample sizes, could lead to the
179 opposite (negative) association between MD activity level and behavior as has been
180 reported in the literature. These results align well with findings from lesion studies that
181 have suggested that a substantial portion of the variance in executive abilities and fluid

182 intelligence is strongly and selectively associated with frontal and parietal MD brain
183 regions.

184 **Materials and Methods**

185 **Participants**

186 216 participants (age 23.6 ± 6.4 , 136 males, 190 right handed, 13 left handed, 8
187 ambidextrous, 5 with missing handedness data) with normal or corrected-to-normal
188 vision, students at Massachusetts Institute of Technology (MIT) and members of the
189 surrounding community, participated for payment. All participants gave informed
190 consent in accordance with the requirements of the Committee On the Use of Humans
191 as Experimental Subjects (COUHES) at MIT.

192 **Experimental Paradigms**

193 Participants performed a spatial working memory task in a blocked design (**Fig. 1**).
194 Each trial lasted 8 seconds: within a 3x4 grid, a set of locations lit up in blue, one at a
195 time for a total of 4 (easy condition) or two at a time for a total of 8 (hard condition).
196 Participants were asked to keep track of the locations. At the end of each trial, they
197 were shown two grids with some locations lit up and asked to choose the grid that
198 showed the correct, previously shown locations by pressing one of two buttons. They
199 received feedback on whether they answered correctly. Each participant performed two
200 runs, with each run consisting of six 32-second easy condition blocks, six 32-second
201 hard condition blocks, and four 16-second fixation blocks, for a total duration of 448s
202 (7min 28s). Condition order was counterbalanced across runs.

203 In addition to the spatial working memory task, all participants performed a
204 language localizer task (Fedorenko et al., 2010), used here to test the selectivity of the
205 relationship between the MD network's activity and behavior. The majority of the
206 participants (n=182, 84.3%) passively read sentences and lists of pronounceable
207 nonwords in a blocked design (see Table 1). The Sentences>Nonwords (S>N) contrast
208 targets brain regions sensitive to high-level linguistic processing (Fedorenko et al.,
209 2011, 2010). Each trial started with 100ms pre-trial fixation, followed by a 12-word-long
210 sentence or a list of 12 nonwords presented on the screen one word/nonword at a time
211 at the rate of 450ms per word/nonword. Then, a line drawing of a hand pressing a
212 button appeared for 400ms, and participants were instructed to press a button
213 whenever they saw the icon, and finally a blank screen was shown for 100ms, for a total
214 trial duration of 6s. The button-press task was included to help participants stay alert
215 and focused. Each block consisted of 3 trials and lasted 18s. Each participant
216 performed two runs, with each run consisting of sixteen experimental blocks (eight per
217 condition), and five fixation blocks (14s each), for a total duration of 358s (5min 58s).
218 Condition order was counterbalanced across runs. The remaining 21 participants
219 performed similar versions of the language localizer with minor differences in the timing
220 and procedure, with one participant performing an auditory version of the localizer (see
221 Table 1 for exact timings and procedures; we have previously established that the
222 localizer contrast is robust to such differences (Fedorenko et al., 2010; Mahowald &
223 Fedorenko, 2016; Scott, Gallée, & Fedorenko, 2017).

224

225

	Version			
	A	B	C	D
Number of participants	182	12	1	8
Task (Passive Reading/Listening / Memory)	PR	M	PL	M
Words / nonwords per trial	12	12	variable	12
Trial duration (ms)	6,000	6000	18000	6000
Fixation	100	300	0	300
Presentation of each word / nonword	450	350	variable	350
Probe (M) + button press (M/PR)	400	1000	--	1000
Fixation	100	500	0	500
Trials per block	3	3	1	3
Block duration (s)	18	18	18	18
Blocks per condition (per run)	8	8	8	6
Conditions	Sentences Nonwords	Sentences Nonwords	Intact speech Degraded speech	Sentences Nonwords Word-lists (not used here)
Fixation block duration (s)	14	18	14	18
Number of fixation blocks per run	5	5	5	4
Total run time (s)	358	378	358	396
Number of runs	2	2	2	2-3

226

227 **Table 1.** Details of the design, materials, and procedure for the different variants of the
 228 language localizer task.

229

230 Finally, most participants completed one or more additional experiments for
231 unrelated studies. The entire scanning session lasted approximately 2 hours.

232 A subset of 114 participants performed the non-verbal component of KBIT
233 (Kaufman & Kaufman, 2014) after the scanning session. The test consists of 46 items
234 (of increasing difficulty) and includes both meaningful stimuli (people and objects) and
235 abstract ones (designs and symbols). All items require understanding the relationships
236 among the stimuli and have a multiple-choice format. If a participant answers 4
237 questions in a row incorrectly, the test is terminated, and the remaining items are
238 marked as incorrect. The test is scored following the formal guidelines to calculate each
239 participant's IQ score.

240 **MRI data acquisition**

241 Structural and functional data were collected on the whole-body 3 Tesla Siemens Trio
242 scanner with a 32-channel head coil at the Athinoula A. Martinos Imaging Center at the
243 McGovern Institute for Brain Research at MIT. T1-weighted structural images were
244 collected in 128 axial slices with 1mm isotropic voxels (TR=2,530ms, TE=3.48ms).
245 Functional, blood oxygenation level dependent (BOLD) data were acquired using an
246 EPI sequence (with a 90° flip angle and using GRAPPA with an acceleration factor of
247 2), with the following acquisition parameters: thirty-one 4mm thick near-axial slices,
248 acquired in an interleaved order with a 10% distance factor; 2.1mm x 2.1mm in-plane
249 resolution; field of view of 200mm in the phase encoding anterior to posterior (A > P)
250 direction; matrix size of 96mm x 96mm; TR of 2,000ms; and TE of 30ms. Prospective
251 acquisition correction (Thesen, Heid, Mueller, & Schad, 2000) was used to adjust the

252 positions of the gradients based on the participant's motion one TR back. The first 10s
253 of each run were excluded to allow for steady-state magnetization.

254 **FMRI data preprocessing and first-level analysis**

255 FMRI data were analyzed using SPM5 and custom MATLAB scripts in volume space.
256 (Note that first-level analyses have not changed much in later versions of SPM; we used
257 an older version of the software here due to the use of these data in other projects
258 spanning many years and hundreds of subjects; critical second-level analyses were
259 performed using custom MATLAB scripts. We also verified using an independent
260 dataset that estimates of neural activity extracted with SPM5- vs. SPM12-preprocessed
261 and modeled data were extremely similar). Each subject's data were motion corrected
262 and then normalized into a common brain space (the Montreal Neurological Institute
263 (MNI) template) and resampled into 2mm isotropic voxels. The data were then
264 smoothed with a 4mm Gaussian filter (FWHM) and high-pass filtered (at 200s). The task
265 effects in both the spatial WM task and in the language localizer task were estimated
266 using a General Linear Model (GLM) in which each experimental condition was
267 modeled with a separate boxcar regressor (with boxcars corresponding to blocks). For
268 the working memory task, each run was modelled by one regressor for the easy blocks
269 and one regressor for the hard blocks; similarly for the language task, each run was
270 modelled by one regressor for sentence blocks and one regressor for non-word blocks.
271 Regressors were convolved with the canonical hemodynamic response function (HRF).
272 The model also included first-order temporal derivatives of these effects, as well as
273 nuisance regressors representing entire experimental runs and offline-estimated motion
274 parameters.

275 Fixation blocks in both tasks were not modeled and treated as the implicit baseline.

276 **MD fROIs definition and response estimation**

277 To define the MD and language (see below) functional regions of interest (fROIs), we
278 used the Group-constrained Subject-Specific (GSS) approach (Fedorenko et al., 2010).
279 In particular, fROIs were constrained to fall within a set of “masks”, areas that
280 corresponded to the expected gross locations of activation for the relevant contrast. For
281 the MD fROIs, following Fedorenko et al. (Fedorenko et al., 2013) and Blank et al.
282 (Blank et al., 2014), we used eighteen anatomical masks (Tzourio-Mazoyer et al., 2002)
283 across the two hemispheres. These masks covered the portions of the frontal and
284 parietal cortices where MD activity has been previously reported, including bilateral
285 opercular inferior frontal gyrus (L/R IFGop), middle frontal gyrus (L/R MFG), orbital MFG
286 (L/R MFGorb), insular cortex (L/R Insula), precentral gyrus (L/R PrecG), supplementary
287 and presupplementary motor areas (L/R SMA), inferior parietal cortex (L/R ParInf),
288 superior parietal cortex (L/R ParSup), and anterior cingulate cortex (L/R ACC) (**Fig. 2a**).
289 It is worth noting, however, that a whole-brain GSS analysis (Fedorenko et al., 2010)
290 performed on the Hard>Easy spatial WM activation maps of n=197 participants yields a
291 set of functional masks that largely overlap with these anatomical parcels (e.g. Diachek
292 et al., 2020). Within each mask, we selected the top 10% (as well as the top 20% and
293 30% for validation analyses, as described below) of most responsive voxels in each
294 individual participant based on the *t*-values for the H>E spatial WM contrast. This top
295 n% approach ensures that each fROI can be defined in every participant, and that the
296 fROI sizes are identical across participants.

297 To estimate the fROIs' responses to the Hard and Easy conditions, we used an
298 across-run cross-validation procedure (Nieto-Castañón & Fedorenko, 2012) to ensure
299 that the data used to identify the fROIs are independent from the data used to estimate
300 their response magnitudes (Kriegeskorte, Simmons, Bellgowan, & Baker, 2009). To do
301 this, the first run was used to define the fROIs and the second run to estimate the
302 responses. This procedure was then repeated using the second run to define the fROIs
303 and the first run to estimate the responses. Finally, the responses were averaged
304 across the left-out runs to derive a single response magnitude estimate for each
305 participant in each fROI for each condition. Finally, these estimates were averaged
306 across the 18 fROIs of the MD network to derive one value per condition for each
307 participant (see **Fig. 2c** for evidence of strong inter-region correlations in effect sizes,
308 replicating Mineroff et al., 2018). (An alternative approach could have been to examine
309 fROI *volumes* – the number of MD-responsive voxels at a fixed significance threshold –
310 instead of effect sizes. However, first, effect sizes and region volumes are strongly
311 correlated; and second, effect sizes tend to be more stable within participants than
312 region volumes (Mahowald & Fedorenko, 2016)).

313 **Language fROIs definition and response estimation**

314 To define the language fROIs, we used a set of six functional masks that were
315 generated based on a group-level representation of data for the Sentences>Nonwords
316 contrast from a large set (n=220) of participants (e.g., Paunov et al., 2019). These
317 masks included three regions in the left frontal cortex: two located in the inferior frontal
318 gyrus, and one located in the middle frontal gyrus; and three regions in the left temporal
319 and parietal cortices spanning the entire extent of the lateral temporal lobe and going

320 posteriorly to the angular gyrus. Within each masks, we selected the top 10% of most
321 responsive voxels in each individual participant based on the *t*-values for the
322 Sentences>Nonwords contrast. To estimate the fROIs' responses to the Sentences and
323 Nonwords conditions, we used the across-run cross-validation procedure described
324 above.

325 **Data availability**

326 Stimuli presentation codes, analysis codes and data (behavioral measures, activation
327 beta estimates and brain maps) are available at <https://osf.io/2tw6j/>. Access to raw data
328 can be requested by e-mailing E.F.

329

330 Results

331 Reliability of behavioral measures

332 Behavioral performance on the spatial WM task was as expected: individuals were more
333 accurate and faster on the easy trials (accuracy=92.22% \pm 7.88%; RT=1.20s \pm 0.23s)
334 than the hard trials (accuracy=77.47% \pm 11.10%, $t_{(215)}=-23.23$, $p<0.0001$, Cohen's
335 $d=1.53$ (effect sizes are based on the two-tailed independent samples t -test); RT=1.49s
336 \pm 0.25s, $t_{(215)}=-26.14$, $p<0.0001$, Cohen's $d=-1.23$). Behavioral measures were stable
337 within individuals across runs for overall (averaging across the Hard and Easy
338 conditions) accuracies ($r=0.66$, $p<0.0001$) and RTs ($r=0.81$, $p<0.0001$). In contrast,
339 difference scores (Hard > Easy) were less stable for both accuracies ($r=0.26$, $p<0.0001$)
340 and RTs ($r=0.46$, $p<0.0001$) (**Fig. 1**). To further validate overall scores as a reliable
341 individual measure (i.e., stable across runs within an individual), we tested their
342 correlation with IQ scores, a well-established stable measure, in the subset of subjects
343 ($n=114$) that performed the IQ KBIT test. Indeed, IQ scores correlated with overall but
344 not difference accuracy scores ($r(\text{IQ vs. overall})=0.35$ vs. $r(\text{IQ vs. H>E})=0.0033$)
345 whereas the correlations were similar for RTs ($r(\text{IQ vs. overall})=-0.21$ vs. $r(\text{IQ vs.}$
346 $\text{H>E})=0.22$). Thus, in the critical brain-behavior analyses below, we used overall
347 accuracies and RTs rather than the H>E measures, because the former are more stable
348 within individuals as demonstrated by their high correlation across runs and correlation
349 with the well-established stable IQ measure. Furthermore, the H>E behavioral
350 measures might contain a non-linearity, such that smaller between-condition differences
351 are observed in both high performers (when performance is close to ceiling) and low
352 performers (when performance is close to chance).

359 **MD network activity and behavior**

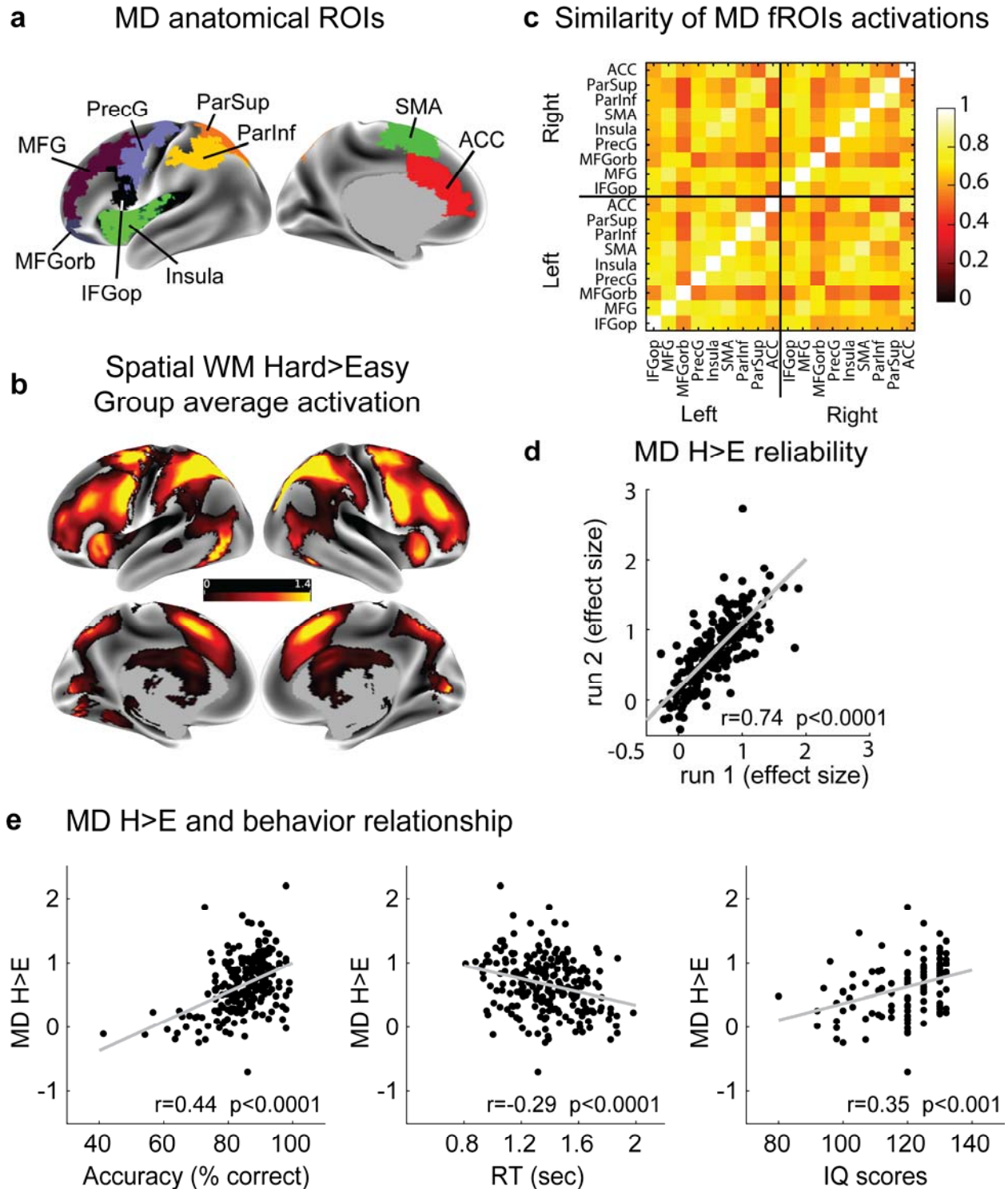
360 As expected (Fedorenko et al., 2013), each of the eighteen MD fROIs individually, as
361 well the MD network as a whole (averaging across fROIs), showed a highly robust H>E
362 effect across participants separately in each run ($t_{(215)} > 11.54$, $p < 0.0001$, Cohen's
363 $d = 0.79-1.54$). Individual differences in the MD H>E effect sizes were also stable across
364 runs for each MD fROI individually ($r = 0.60-0.80$) and when averaging across fROIs
365 ($r = 0.74$, $p < 0.0001$; **Fig. 2d**). We used the H>E contrast as it was more stable than
366 task>fixation contrasts (H>fix $r = 0.65$ and E>fix $r = 0.31$). This greater stability of the H>E
367 contrast plausibly reflects the fact that it factors out variability due to state differences,
368 thus honing in on the relevant variability, related to the level of the MD network's
369 activity. For each participant, we averaged the H>E effect size across the 18 MD fROIs
370 to derive a single measure because the H>E effect sizes were strongly correlated
371 across the 18 regions ($r = 0.45-0.88$; **Fig. 2c**), replicating Mineroff et al., 2018, and in
372 line with general evidence of the MD brain regions forming a tightly functionally
373 integrated system (Assem et al., 2020; Blank et al., 2014; Paunov et al., 2019).

374 To ensure that the stability of the MD H>E effect size did not depend on the
375 particular details of the fROI definition (i.e., top 10% of most responsive voxels within
376 the masks), we also extracted the effect sizes from the fROIs defined as the top 20%
377 and top 30% of most responsive voxels. The extracted H>E effect sizes were almost
378 perfectly correlated with those extracted from the top 10% fROIs (20% vs 10%, $r = 0.99$,
379 $p < 0.0001$; 30% vs 10%, $r = 0.98$, $p < 0.0001$). Thus, we proceed to use the H>E effect
380 sizes extracted from the original (10%) fROIs.

381 For each participant, we used behavioral measures from the spatial WM task
382 (overall accuracies and RTs), and one brain activation measure (H>E effect sizes
383 averaged across the 18 MD ROIs). The critical analyses revealed that larger MD H>E
384 effect sizes were associated with more accurate (Pearson's $r=0.44$, Spearman's $r=0.42$,
385 both $ps<0.0001$) and faster (Pearson's $r=-0.29$, Spearman's $r=-0.29$, both $ps<0.0001$;
386 **Fig. 2e**) performance. To further test the predictive power of MD H>E effect sizes, we
387 cross-compared brain-behavior relationships across runs (Dubois & Adolphs, 2016) and
388 found that MD H>E effect sizes in run 1 correlated with both accuracies (Pearson's
389 $r=0.34$, Spearman's $r=0.33$, both $ps<0.0001$) and RTs (Pearson's $r=-0.22$, Spearman's
390 $r=-0.26$, both $ps<0.0001$) in run 2, and MD H>E effect sizes in run 2 correlated with
391 accuracies (Pearson's $r=0.40$, Spearman's $r=0.38$, both $ps<0.0001$) and RTs (Pearson's
392 $r=-0.27$, Spearman's $r=-0.27$, both $ps<0.0001$) in Run 1.

393 Next, to test the generalizability of the relationship between MD activation and
394 behavior, we asked whether MD H>E effect sizes explain variance in fluid intelligence,
395 as measured with the Kaufman Brief Intelligence Test (KBIT) (Kaufman & Kaufman,
396 2014) in a subset of participants ($n=114$). Indeed, larger MD H>E effect sizes were
397 associated with higher intelligence quotient (IQ) scores (Pearson's $r=0.34$, $p<0.0002$,
398 normalized $R^2(R^2_{H>E \text{ vs IQ}}/R^2_{H>E \text{ reliability}})=21\%$; Spearman's $r=0.41$, $p<0.0001$ **Fig. 2e**).
399 This relationship was still significant after controlling for WM accuracy using a partial
400 correlation analysis (Pearson's $r=0.26$, $p=0.0061$; Spearman's $r=0.34$, $p=0.0003$),
401 suggesting that MD activity explains unique variance captured by the fluid intelligence
402 test over and above any shared working memory component between the test and the
403 task.

404 These results thus support a positive association between MD activity and fluid
405 cognitive abilities. In the next section we assess the selectivity of this MD-behavior
406 relationship.
407



408

409 **Figure 2. MD activity and behavior. (a)** Surface projection of the volumetric

410 anatomical masks used to constrain individual-specific functional activations. **(b)**

411 Surface projection of the volumetric unthresholded group average activation map (beta
412 estimates) for the spatial WM Hard>Easy (H>E) contrast. Please note that all analyses
413 were performed in volume space, and surface projections—here and in other figures—
414 are for illustrative purposes only and may include slight distortions resulting from
415 volume-to-surface transformations. (Surface projection was performed using
416 Connectome Workbench (humanconnectome.org/software/connectome-workbench)
417 function “-volume-to-surface-mapping” using trilinear interpolation and a MNI
418 reconstructed mid-thickness surface and displayed on an inflated HCP surface
419 (<https://balsa.wustl.edu/reference/show/pkXDZ>).) **(c)** Pearson correlation (see text for
420 highly similar Spearman values) between MD regions for the H>E contrast, computed
421 across individuals (n = 216). **(d)** Stability of MD H>E effect sizes across runs across
422 individuals (n = 216). **(e)** MD H>E effect sizes and behavior relationship: larger MD H>E
423 effect sizes are associated with better accuracy (*left*) and faster RTs (*middle*) in the
424 spatial WM task (n = 216), as well as higher IQ scores (n = 114) (*right*) as measured by
425 an independent test (KBIT).
426

427 **Language network activity and behavior**

428 Does the strength of brain activity outside of the MD network explain variance in
429 executive abilities? We tested the selectivity of the MD-behavior relationship by
430 examining another large-scale network implicated in high-level cognition: the fronto-
431 temporal language-selective network in the left hemisphere (Fedorenko et al., 2011).

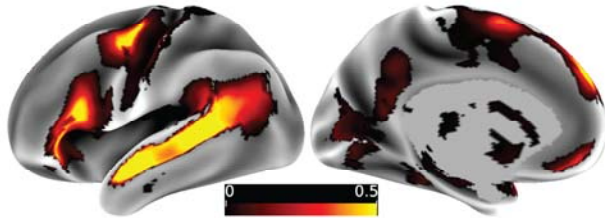
432 We extracted the language network's activity during a reading task (Fedorenko et
433 al., 2010) (Sentences>Nonwords (S>N) contrast; **Fig. 3a**). Similar to MD H>E effect
434 sizes, language S>N effect sizes were highly stable across runs for each language fROI
435 individually and averaging across fROIs ($r=0.83$, $p<0.0001$; **Fig. 3b**), in line with prior
436 work (Mahowald & Fedorenko, 2016; Mineroff et al., 2018).

437 Larger language S>N effect sizes were weakly associated with more accurate
438 (Pearson's $r=0.18$, $p<0.01$; Spearman's $r=0.17$, $p=0.01$) but not faster (Pearson's $r=-$
439 0.08 , $p=0.24$; Spearman's $r=-0.10$, $p=0.14$) performance on the spatial WM task (**Fig.**
440 **3c**). We also observed a weak trend for a relationship between S>N effect sizes and IQ
441 scores (Pearson's $r=0.16$, $p=0.09$; Spearman's $r=0.15$, $p=0.11$) (**Fig. 3c**). Critically,
442 however, controlling for the size of the MD H>E effects, in a partial correlation analysis,
443 abolished the associations between language S>N effect sizes and the behavioral
444 measures (spatial WM accuracies: Pearson's $r=0.11$, $p=0.10$, Spearman's $r=0.18$,
445 $p=0.09$; IQ scores: Pearson's $r=0.14$, $p=0.14$, Spearman's $r=0.11$, $p=0.25$; **Fig. 3d**). In
446 contrast, controlling for the size of the language S>N effects did not affect the
447 relationship between MD H>E effect sizes and the behavioral measures (spatial WM
448 accuracies: Pearson's $r=0.42$ cf. $r=0.44$; spatial WM RTs: Pearson's $r=-0.27$ cf. $r=-0.29$;
449 IQ scores: Pearson's $r=0.34$ cf. $r=0.35$; all $ps<0.001$).

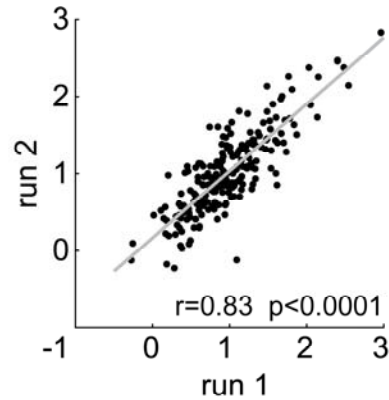
450 In line with findings from brain lesion studies, these results confirm the selective
451 relationship between the MD network and executive functions / fluid intelligence.

452

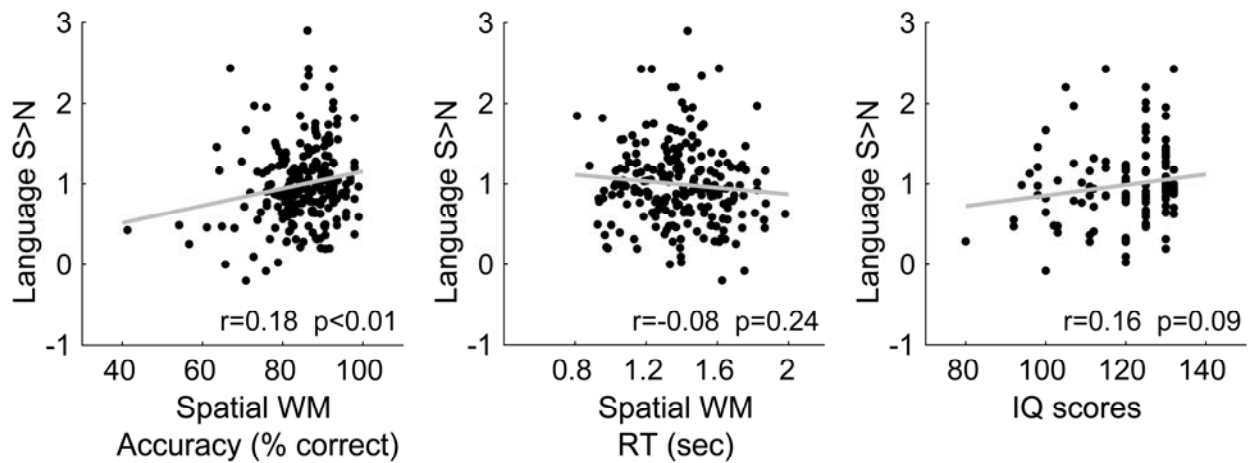
a Language Sentences>Non-words
Group average activation



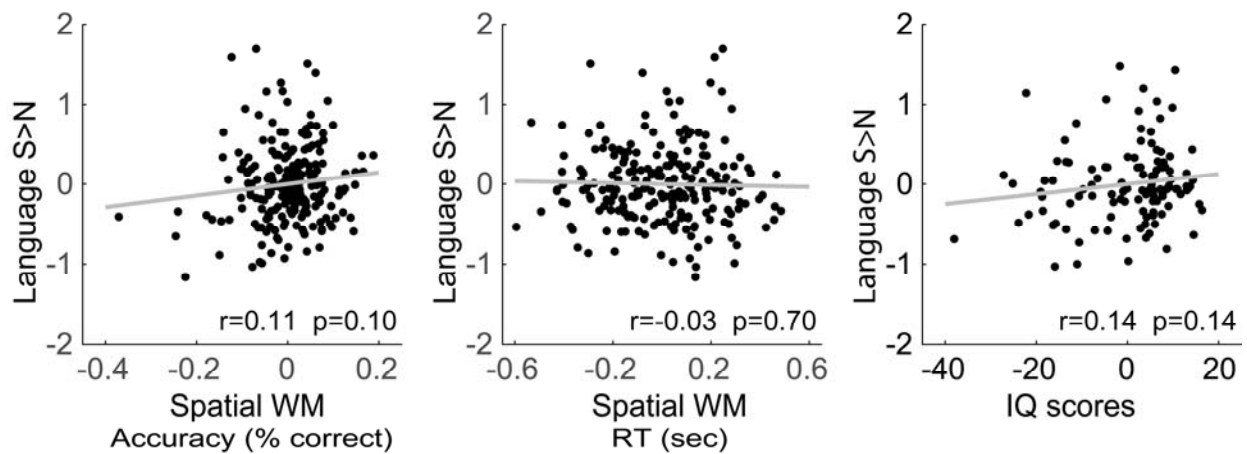
b Language S>N reliability



c Language S>N and behavior relationship



d After controlling for MD H>E activity



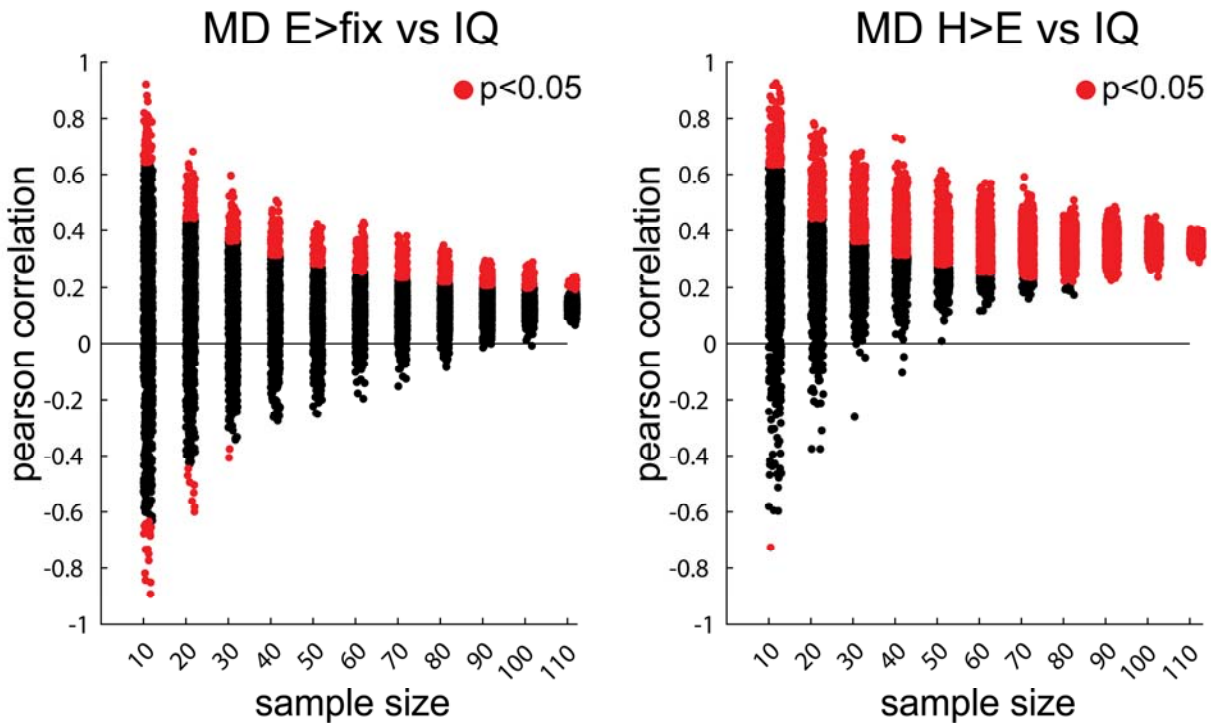
454 **Figure 3. Language network activity and behavior. (a)** Surface projection of the
455 volumetric unthresholded group average activation map (beta estimates) for the
456 language Sentences>Nonwords (S>N) contrast. **(b)** Stability of language S>N effect
457 sizes across runs across individuals (n=216) (Pearson correlations are used in the
458 figures; see text for highly similar Spearman values). **(c)** Language S>N effect sizes and
459 behavior relationship: larger language S>N effect sizes are weakly associated with
460 better accuracy in the spatial WM task (*left*) and higher IQ scores (*right*), but not RTs in
461 the WM task (*middle*). **(d)** Language S>N effect sizes and behavior relationship,
462 controlling for MD H>E effect sizes: the weak relationships between language S>N
463 effect sizes and behavior observed in (c) are now abolished.

464 **Effect of sample size and reliability of the fMRI activity on brain-** 465 **behavior associations**

466 In a further attempt to explain discrepancies in the prior literature (e.g., some studies
467 finding that stronger MD activity is associated with better executive abilities, but other
468 studies finding the opposite pattern, as discussed in the Introduction), we examined the
469 effects of sample size and reliability of the fMRI effect sizes on the brain-behavior
470 relationships (Gelman & Carlin, 2014). We used two indices of MD activity that differed
471 in their reliability – (1) MD H>E effect size used in the main analysis above (a highly
472 reliable measure, with the across-runs correlation of Pearson's $r=0.74$) and (2) MD
473 E>Fix effect size (a less reliable measure, with the across-runs correlation of Pearson's
474 $r=0.31$) – and examined their relationship to IQ scores.

475 Samples of different sizes (ranging from 10 to 110, in increments of 10) were
476 randomly selected from our set of 114 participants. For each sample, we computed a
477 correlation between each of the two activity measures and IQ scores. This process was
478 repeated 1,000 times per sample size. The resulting correlations were then examined
479 for their sign, size, and significance. The results, shown in **Fig. 4 (left)**, clearly
480 demonstrate that a combination of small samples and brain activity measures of low
481 reliability (e.g., MD E>fix effect size), like those used in many earlier studies, can
482 produce a significant ($p<0.05$) correlation of the opposite sign to that observed in a
483 larger population (red dots with a negative correlation). This problem is diminished, but
484 not eliminated, when a reliable index like the MD H>E effect size is used (**Fig. 4, right**).
485 The results also demonstrate that inflated correlations that are often observed in small
486 samples are not eliminated even when a reliable activity measure is used.

487 The results from this analysis also challenge the claim of a negative association
488 between MD activity and performance observed in easier tasks. As demonstrated
489 above, at least in this paradigm, brain activity during a relatively easy executive task
490 was not reliable within individuals across runs. This low reliability could yield
491 correlations of opposite sign. However, even with large sample sizes, the MD E>fix
492 effect size shows a weak positive, not negative, association with IQ scores (**Fig. 4, left**).
493



494

495 **Figure 4. Effects of sample size and the reliability of the brain measure on brain-**
496 **behavior relationships.** On the x-axis in both panels, we show correlations (1,000 per
497 sample) obtained for samples of different sizes. In the left panel, we use a brain activity
498 measure of low reliability (MD E>Fix effect size), and in the right panel, we use a highly
499 reliable brain activity measure (MD H>E effect size). Correlations significant at the
500 $p < 0.05$ level are marked in red.

501

502 Discussion

503 In a large set of participants, we examined the relationship between activity in the
504 fronto-parietal “multiple-demand (MD)” network (Duncan, 2010, 2013), on the one hand,
505 and executive abilities and fluid intelligence, on the other. The brain regions of interest
506 were defined in individuals using a functional localizer task (e.g. Fedorenko et al.,
507 2013). We observed a robust positive association between the strength of activation in
508 the MD network and performance on a spatial working memory (WM) task in the
509 scanner, as well as IQ measured independently. We also examined the specificity of
510 this relationship by considering another network important for high-level cognition – the
511 fronto-temporal language-selective network (Fedorenko et al., 2011). Although the
512 strength of activation in this network showed a weak positive association with some of
513 the behavioral measures, these relationships were eliminated once the level of the MD
514 network’s activity was taken into account (controlling for the level of the language
515 network’s activity did not affect the MD-behavior relationships). Finally, we showed how
516 small sample sizes and/or the use of brain activity measures of low reliability, as used in
517 many earlier studies (Dunst et al., 2014; Haier et al., 1988; Lipp et al., 2012; Rypma et
518 al., 2006), could produce inflated and/or the opposite-sign correlations between brain
519 and behavior. To our knowledge, our relatively large sample size, coupled with the
520 participant-specific functional localization approach to defining the regions of interest
521 (Nieto-Castañón & Fedorenko, 2012; Saxe et al., 2006), provides the strongest
522 evidence to date for a positive association between the MD network’s activity and
523 behavioral measures of executive abilities and fluid intelligence. This evidence aligns
524 well with findings from lesion studies that have also reported a selective relationship

525 between fronto-parietal regions and fluid cognitive abilities (Duncan et al., 1995;
526 Glascher et al., 2010; Roca et al., 2010; Warren et al., 2014; Woolgar et al., 2018,
527 2010).

528 **Constraints on generality**

529 Some limitations for our study are worth noting (Simons, Shoda, & Lindsay, 2017). First,
530 some researchers have previously tried to explain the discrepancies in the MD-behavior
531 literature by alluding to differences in the age of participants across studies (Reuter-
532 Lorenz et al., 2000; Rypma & Esposito, 2000), arguing that the MD-behavior
533 relationship may change across the lifespan. These changes may be driven by
534 processes like cognitive reserve and brain maintenance in old age (Nyberg & Pudas,
535 2019; Sala-Llonch, Bartres-Faz, & Junque, 2015; Stern, 2017) or reorganization of
536 neurocognitive architecture in adolescents (Simpson-Kent et al., 2020). The age range
537 in our sample (25th-75th percentile = 20-25) is too narrow to evaluate this hypothesis
538 rigorously. That said, the early studies that had motivated this hypothesis a) used small
539 sample sizes (e.g. Rypma and Esposito, 2000), b) used task>fixation activation
540 measures that are likely to be unreliable, and c) did not take into account inter-individual
541 variability in the locations of the MD regions, which may be especially important given
542 the increased variability in the functional architecture of older adults (Geerligs,
543 Tsvetanov, Cam-CAN, & Henson, 2017).

544 Second, as briefly mentioned in the introduction, some researchers have argued
545 that negative MD-behavior associations can be observed during some easy tasks. For
546 example, a recent study using the HCP n-back task (Barch et al., 2013) demonstrates
547 that whereas MD activations during the 2-back condition are positively associated with

548 general intelligence, MD activations during the 0-back condition show a negative
549 association (Sripada et al., 2020). It is plausible that our easy condition is more
550 cognitively demanding than the 0-back condition, and that is why we did not observe a
551 negative correlation between the E>Fix activations and IQ scores (**Fig. 4, left**).

552 More broadly, there are situations where improvement in performance is
553 associated with decreases in MD activity e.g. in paradigms with extended motor skills
554 practice (Dayan & Cohen, 2011; Steele & Penhune, 2010) or task rules practice
555 (Hampshire et al., 2019; Ruge & Wolfensteller, 2010). In such cases, efficient
556 performance is plausibly mediated by re-configuration of brain processes. Extended
557 practice can be conceived as a shift from a novel (hard) task to a routine (easy) task.
558 Shifts from hard to easy tasks are known to be associated with anterior to posterior
559 shifts in peak MD activations (Assem et al., 2020; Badre, 2008; Crittenden & Duncan,
560 2014; Shashidhara, Mitchell, Erez, & Duncan, 2019). Thus, MD activation decreases
561 with practice could reflect these hard to easy topographical activation shifts.

562 Third, our study used MD activity estimates during a single task. An estimate
563 derived from multiple MD tasks may more accurately capture the variability in the MD
564 network's engagement across individuals. Similarly, our measure of fluid intelligence
565 was derived from a single IQ test (KBIT; Kaufman and Kaufman, 2013). A measure of
566 fluid intelligence based on a diverse battery of executive function tasks may be more
567 reliable. Nevertheless, we note that in our study (a) the size of the correlation we
568 observed ($r \sim -0.35$) is within the range of correlations reported in recent studies that
569 have used a multi-task-based estimate of fluid intelligence (Dubois et al., 2018; Sripada
570 et al., 2020), (b) the relation between MD-IQ survived after controlling for the correlation

571 between IQ and WM performance, highlighting the unique behavioral variance captured
572 by the KBIT test over and above the WM task.

573 **MD system activation and intelligence**

574 We estimated MD activity using a blocked design experiment, thus averaging across
575 multiple cognitive processes (in our case, encoding of information into working memory,
576 maintaining and dynamically updating it, and finally, retrieving it from working memory at
577 the decision-making step). Temporally finer-grained MD activity estimates at particular
578 steps in an executive-function task may more precisely target the core neural
579 computations that relate to executive abilities / fluid intelligence. For instance, a recent
580 event-related study demonstrated robust MD activity at each of the stages above
581 (Soreq, Leech, & Hampshire, 2019). Stronger MD activation during more difficult tasks
582 is thought to reflect the increased demand on integrating more and/or different kinds of
583 information in a focused attentional structure to solve the task at hand (Assem et al.,
584 2020; Duncan, 2013). For example, in a recent event-related study, individuals with
585 lower intelligence scores, compared to those with higher scores, showed weaker MD
586 activity during the critical step of target detection suggesting a failure to correctly
587 integrate task rules in the attentional structure guiding successful behavior
588 (Tschantscher et al., 2017). Thus, stronger MD activity across an entire block could
589 plausibly reflect less frequent lapses of “attentional focus” – needed for the correct
590 binding of information to solve the task at hand – and thus better behavioral
591 performance.

592 A general challenge with individual-level estimates from event-related designs is
593 that they are likely to be more noisy / less reliable, although with sufficient data per

594 participant, this limitation could be overcome. An early study (Gray et al., 2003) with 60
595 participants found a significant difference between higher and lower IQ individuals in
596 MD activity when it was estimated from individual lure trials (in a n-back task) but not
597 when MD activity was estimated across an entire block of trials. In our study, we
598 demonstrate that MD activity estimated from a block of trials carries meaningful
599 variance about individual differences in executive performance and fluid intelligence.

600 **Relationship of executive abilities with language and other non-MD regions**

601 Studies of brain lesions have demonstrated repeatedly that there is no relation between
602 lesions in the language network and executive abilities (Fedorenko and Varley, 2016;
603 Woolgar et al., 2018; cf. Baldo et al., 2010). To our knowledge, this is the first study to
604 investigate the relationship between brain activity in the language network and
605 executive abilities / intelligence employing a large sample size and individual-subject
606 fROIs. In line with lesion findings, we show that controlling for MD activity abolishes any
607 relationship between activity in the language network and spatial WM performance and
608 IQ scores. The weak language-behavior association observed prior to controlling for MD
609 activity is plausibly related to a trait factor like vascularization, or a state factor like
610 arousal.

611 More generally, as we have briefly alluded to in the introduction, several studies
612 have linked executive abilities and fluid intelligence to diverse structural and functional
613 brain measures, including outside the boundaries of the MD network. For example, a
614 recent large-scale study using the UK Biobank dataset (n~30,000) reported that total
615 brain volume, as well as multiple global measures of grey and white matter macro- and
616 microstructure (especially, in older participants), explained substantial variance in fluid

617 intelligence (Cox, Ritchie, Fawns-Ritchie, Tucker-Drob, & Deary, 2019). Another study
618 used the HCP task fMRI dataset to show that task-related activations in many brain
619 regions correlates to some extent with general intelligence. However, executive tasks
620 engaging MD regions were the best predictors of individual differences in general
621 intelligence (Sripada et al., 2020), in line with our findings. The relationship among the
622 different neural measures that have been shown to predict variation in fluid intelligence,
623 including the one used in the current study (i.e., the relative increase in the MD activity
624 for a more difficult compared to an easier version of an executive task), is not known.
625 Further studies that assess the reliability of those diverse brain measures, extracted
626 with analysis pipelines that respect inter-individual variability in structure (Kharabian
627 Masouleh, Eickhoff, Hoffstaedter, & Genon, 2019) and function (Coalson, Essen, &
628 Glasser, 2018; Nieto-Castañón & Fedorenko, 2012), and direct comparisons among
629 those measures can help clarify their unique and shared contributions to explaining
630 variability in executive abilities and intelligence. Given the complexity of human
631 reasoning abilities, multiple brain processes likely contribute, but we suggest that the
632 MD network is a key player governing individual differences in fluid intelligence and
633 executive abilities, in line with the fact that damage to MD structures selectively and
634 robustly predicts intelligence losses.

635 **Implications for future studies**

636 There are many long-recognized challenges facing brain-behavior individual-differences
637 studies (Dubois & Adolphs, 2016). In the introduction we highlighted the critical role of
638 individually defined functional regions to correctly delineate brain-behavior relationships.
639 Another challenge concerns small sample sizes. Our results demonstrate that typical

640 sample sizes (n=10-30) in neuroimaging studies can produce misleading and highly
641 inflated brain-behavior correlations. This presents a significant challenge for laboratory-
642 based research, clinical studies with difficult to recruit patients and longitudinal studies
643 that opt for multiple scanning sessions at the expense of increasing sample size.

644 We also demonstrate how unreliable brain or behavioral measures (i.e. not stable
645 within an individual across runs/sessions) can result in invalid and inflated correlations.
646 Reliability can also be compromised by using tasks that do not generate enough
647 between-individuals variance (Hedge, Powell, & Sumner, 2018). This is a general
648 challenge facing integrating experimental and individual differences approaches. For
649 example, response inhibition tasks (e.g. stroop, Go/No-Go) produce replicable
650 experimental effects yet studies on individual differences in performance on these tasks
651 commonly fail to group them in a single construct (Hedge et al., 2018; Rey-Mermet,
652 Gade, Souza, von Bastian, & Oberauer, 2019) or relate them reliably to common brain
653 mechanisms (Rosenberg et al., 2019; Wager et al., 2005).

654 **Conclusions**

655 Against a backdrop of contradictory prior findings, we demonstrate a robust positive and
656 selective association between the MD network's activity level, on the one hand, and
657 executive abilities and fluid intelligence, on the other. Our analyses also help resolve
658 some of the prior contradictions in the literature. Given its high reliability, the MD activity
659 measure used here, and measures obtained from similarly strong manipulations of
660 cognitive demand, can be used as a neural marker to further probe variability in
661 executive abilities both in the typical population and among individuals with cognitive
662 and psychiatric disorders. This marker can also serve as a promising neural bridge

663 (Braver, Cole, & Yarkoni, 2010) between behavioral variability and genetic variability
664 associated with differences in fluid intelligence (Deary, Spinath, & Bates, 2006; Plomin
665 & Spinath, 2004).
666

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678 **Declarations of interest**

679 None

680 **Author Contributions (CRediT Taxonomy)**

681 **M.A.** Conceptualization; Data curation; Formal analysis; Software; Methodology;
682 Visualization; Validation; Writing - original draft; Writing - review & editing.

683 **I.A.B.** Data curation; Formal analysis; Software; Methodology; Investigation; Validation
684 Writing - review & editing.

685 **Z.M.** Data curation; Formal analysis; Software; Investigation; Project administration.

686 **A.A.** Methodology; Supervision; Writing - review & editing.

687 **E.F.** Conceptualization; Data curation; Formal analysis; Funding acquisition;
688 Investigation; Methodology; Project administration; Resources; Software; Supervision;
689 Validation; Roles/Writing - original draft; Writing - review & editing.

690

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