Decoding across sensory modalities reveals common supramodal signatures of conscious perception

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Abstract

An increasing number of studies highlight the role of fronto-parietal brain structures in mediating conscious sensory experience. While most studies have been performed in the visual modality, it is implicitly assumed that similar processes are involved in other sensory modalities. However, the existence of supramodal neural processes related to conscious perception has not been convincingly shown so far. Here, we aim to directly address this issue by investigating whether neural correlates of conscious perception in one modality can predict conscious perception in a different modality. In two separate experiments, we presented participants with successive blocks of near-threshold tasks involving tactile, visual or auditory stimuli during the same magnetoencephalography (MEG) acquisition. Using decoding analysis in the post-stimulus period between sensory modalities, the first experiment uncovered supramodal spatio-temporal neural activity patterns predicting conscious perception of the feeble stimulation. Strikingly, these supramodal patterns included late activity in primary sensory regions not directly relevant to the task (e.g. neural activity in visual cortex predicting conscious perception of auditory near-threshold stimulation). We carefully replicate our results in a control experiment that furthermore show that the relevant patterns are independent of the type of report (i.e. whether conscious perception was reported by pressing or withholding a button-press). Using standard paradigms for probing neural correlates of conscious perception, our findings reveal a common signature of conscious access across sensory modalities and illustrate the temporally late and widespread broadcasting of neural representations, even into task-unrelated primary sensory processing regions.

Introduction

While the brain can process an enormous amount of sensory information in parallel, only some information can be consciously accessed, playing an important role in the way we perceive and act in our surrounding environment. An outstanding goal in cognitive neuroscience is thus to understand the relationship between neurophysiological processes and conscious experiences. However, despite tremendous research efforts, the precise brain dynamics that enable certain sensory information to be consciously accessed remain unresolved. Nevertheless, progress has been made in research focusing on isolating neural correlates of conscious perception (1), in particular suggesting that conscious perception - at least if operationalized as reportability (2) - of external stimuli crucially depends on the engagement of a widely distributed brain network (3). To study neural processes underlying conscious perception, neuroscientists often expose participants to near-threshold (NT) stimuli that are matched to their individual perceptual thresholds (4). In NT experiments, there is a trial-to-trial variability in which around 50% of the stimuli at NT-intensity are consciously perceived. Because of the fixed intensity, the physical differences between stimuli within the same modality can be excluded as a determining factor leading to reportable sensation (5). Despite numerous methods used to investigate conscious perception of external events, most studies target a single sensory modality. However, any specific neural pattern identified as a correlate of consciousness needs evidence that it generalizes to some extent, e.g. across sensory modalities. We argue that this has not been convincingly shown so far.

In the visual domain, it has been shown that reportable conscious experience is present when primary visual cortical activity extends towards hierarchically downstream brain areas (6), requiring the activation of frontoparietal regions in order to become fully reportable (7). Nevertheless, a recent MEG study using a visual masking task revealed early activity in primary visual cortices as the best predictor for conscious perception (8). Other studies have shown that neural correlates of auditory consciousness relate to the activation of fronto-temporal rather than fronto-parietal networks (9, 10). Additionally, recurrent processing

between primary, secondary somatosensory and premotor cortices have been suggested as

potential neural signatures of tactile conscious perception (11, 12). Indeed, recurrent

processing between higher and lower order cortical regions within a specific sensory system

is theorized to be a marker of conscious processing (6, 13, 14). Moreover, alternative theories

such as the global workspace framework (15) extended by Dehaene et al. (16) postulates that

the frontoparietal engagement aids in 'broadcasting' relevant information throughout the brain,

making it available to various cognitive modules. In various electrophysiological experiments,

it has been shown that this process is relatively late (~300 ms), and could be related to

increased evoked brain activity after stimulus onset such as the so-called P300 signal (17–

19). Such late brain activities seem to correlate with perceptual consciousness and could

reflect the global broadcasting of an integrated stimulus making it conscious. Taken together,

theories and experimental findings argue in favor of various 'signatures' of consciousness from

recurrent activity within sensory regions to a global broadcasting of information with

engagement of fronto-parietal areas. Even though usually implicitly assumed, it is so far

unclear whether similar spatio-temporal neural activity patterns are linked to conscious access

across different sensory modalities.

In the current study, we investigated conscious perception in different sensory systems

using multivariate analysis on MEG data. Our working assumption is that brain activity related

to conscious access has to be independent from the sensory modality: i.e. supramodal

consciousness-related neural processes need to exhibit spatio-temporal generalization. Such

a hypothesis is most ideally tested applying decoding methods to electrophysiological signals

recorded while probing conscious access in different sensory modalities. The application of

multivariate pattern analysis (MVPA) to EEG/MEG measurements offers increased sensitivity

in detecting experimental effects distributed over space and time (20–23). MVPA is often used

in combination with a searchlight method (24, 25), which involves sliding a small spatial

window over the data to reveal areas containing decodable information. The combination of

both methods provides spatio-temporal detection of optimal decodability, determining where,

when and for how long a specific pattern is present in brain activity. Such multivariate decoding

analyses have been proposed as an alternative in consciousness research, complementing

other conventional univariate approaches in order to identify neural activity predictive of

conscious experience at the single trial level (26).

Here, we acquired MEG data while each participant performed three different standard

NT tasks on three sensory modalities with the aim of characterizing supramodal brain

mechanisms of conscious perception. In the first experiment we show how neural patterns

related to perceptual consciousness can be generalized over space and time within and –most

importantly- between different sensory systems by using classification analysis on source-

level reconstructed brain activity. In an additional control experiment, we replicate the main

findings and exclude the possibility that our observed patterns are due to response preparation

/ selection.

Materials and Methods

Participants

Twenty-five healthy volunteers took part in the initial experiment conducted in Trento

and twenty-one healthy volunteers took part in the control experiment performed in Salzburg.

All participants presented normal or corrected-to-normal vision and no neurological or

psychiatric disorders. Three participants for the initial experiment and one participant for the

control experiment were excluded from the analysis due to excessive artifacts in the MEG data

leading to an insufficient number of trials per condition after artifact rejection (less than 30

trials for at least one condition). Additionally, within each experiment six participants were

discarded from the analysis because false alarms rate exceeded 30% and/or near-threshold

detection rate was over 85% or below 15% for at least one sensory modality (due to threshold

identification failure and difficulty to use response button mapping during the control

experiment, also leaving less than 30 trials for at least one relevant condition in one sensory

modality: detected or undetected). The remaining 16 participants (11 females, mean age: 28.8

years; SD: 3.4 years) for the initial experiment and 14 participants (9 females, mean age: 26.4

years; SD: 6.4 years) for the control experiment, reported normal tactile and auditory

perception. The ethics committee of the University of Trento and University of Salzburg

respectively, approved the experimental protocols that were used with the written informed

consent of each participant.

Stimuli

To ensure that the participant did not hear any auditory cues caused by the piezo-

electric stimulator during tactile stimulation, binaural white noise was presented during the

entire experiment (training blocks included). Auditory stimuli were presented binaurally using

MEG-compatible tubal in-ear headphones (SOUNDPixx, VPixx technologies, Canada). Short

bursts of white noise with a length of 50 ms were generated with Matlab and multiplied with a

Hanning window to obtain a soft on- and offset. Participants had to detect short white noise

bursts presented near hearing threshold (27). The intensity of such transient target auditory

stimuli was determined prior to the experiment in order to emerge from the background

constant white noise stimulation. Visual stimuli were Gabor ellipsoid (tilted 45°) back-projected

on a translucent screen by a Propixx DLP projector (VPixx technologies, Canada) at a refresh

rate of 180 frames per second. The stimuli were presented 50 ms in the center of the screen

at a viewing distance of 110 cm. Tactile stimuli were delivered with a 50 ms stimulation to the

tip of the left index finger, using one finger module of a piezo-electric stimulator (Quaerosys,

Schotten, Germany) with 2 × 4 rods, which can be raised to a maximum of 1 mm. The module

was attached to the finger with tape and the participant's left hand was cushioned to prevent

any unintended pressure on the module (28). For the control experiment (conducted in another

laboratory; i.e. Salzburg), visual, auditory and tactile stimulation setups were identical but we

used a different MEG/MRI vibrotactile stimulator system (CM3, Cortical Metrics).

Task and design

The participants performed three blocks of a NT perception task. Each block included

three separate runs (100 trials each) for each sensory modality, tactile (T), auditory (A) and

visual (V). A short break (~1 min) separated each run and longer breaks (~4 min) were

provided to the participants after each block. Inside a block, runs alternated in the same order

within subject and were pseudo-randomized across subjects (i.e. subject 1 = TVA-TVA-TVA;

subject 2 = VAT-VAT-VAT; …). Participants were asked to fixate on a central white dot in a

grey central circle at the center of the screen throughout the whole experiment to minimize

eye movements.

A short training run with 20 trials was conducted to ensure that participants had

understood the task. Then, in three different training sessions prior to the main experiment,

participants' individual perceptual thresholds (tactile, auditory and visual) were determined in

the shielded room. For the initial experiment, a 1-up/1-down staircase procedure with two

randomly interleaved staircases (one up- and one downward) was used with fixed step sizes.

For the control experiment we used a Bayesian active sampling protocol to estimate

psychometric slope and threshold for each participant (29).

The main experiment consisted of a detection task (Figure 1A). At the beginning of

each run, participants were told that on each trial a weak stimulus (tactile, auditory or visual

depending on the run) could be presented at random time intervals. 500 ms after the target

stimulus onset, participants were prompted to indicate whether they had felt the stimulus with

an on-screen question mark (maximal response time: 2 s). Responses were given using MEG-

compatible response boxes with the right index finger and the middle finger (response button

mapping was counterbalanced among participants). Trials were then classified into hits

(detected) and misses (undetected stimulus) according to the participants' answers. Trials with

no response were rejected. Catch (above perceptual threshold stimulation intensity) and Sham

(absent stimulation) trials were used to control false alarms and correct rejection rates across

the experiment. Overall, there were 9 runs with 100 trials each (in total 300 trials for each

sensory modality). Each trial started with a variable interval (1.3–1.8 s, randomly-distributed)

followed by an experimental near-threshold stimulus (80 per run), a sham stimulus (10 per

run) or a catch stimulus (10 per run) of 50 ms each. Each run lasted for approximately 5 min.

The whole experiment lasted for ~1h.

Identical timing parameters were used in the control experiment. However, a specific

response screen design was used to control for motor response mapping. For each trial the

participants must use a different response mapping related to circle's color surrounding the

question mark during response screen. Two colors (blue or yellow) were used and presented

randomly after each trials during the control experiment. One color was associated to the

following response mapping rule: "press the button only if there is a stimulation" (for near-

threshold condition: "detected") and the other color was associated to the opposite response

mapping: "press a button only if there is no stimulation" (for near-threshold condition:

"undetected"). The association between one response mapping and a specific color (blue or

yellow) was fixed for a single participant but was predefined randomly across different

participant. Importantly, by delaying the response-mapping to after the stimulus presentation

in a -for the individual- unpredictable manner, neural patterns during relevant periods

putatively cannot be confounded by response selection / preparation. Both experiments were

programmed in Matlab using the open source Psychophysics Toolbox (30).

MEG data acquisition and preprocessing

MEG was recorded at a sampling rate of 1kHz using a 306-channel (204 first order

planar gradiometers, 102 magnetometers) VectorView MEG system for the first experiment in

Trento, and Triux MEG system for the control experiment in Salzburg (Elekta-Neuromag Ltd.,

Helsinki, Finland) in magnetically shielded room (AK3B, Vakuumschmelze, Hanau, Germany).

Before the experiments, individual head shapes were acquired for each participant including

fiducials (nasion, pre-auricular points) and around 300 digitized points on the scalp with a

Polhemus Fastrak digitizer (Polhemus, Vermont, USA). Head positions of the individual

relative to the MEG sensors were continuously controlled within a run using five coils. Head

movements did not exceed 1 cm within and between blocks.

Data were analyzed using the Fieldtrip toolbox (31) and the CoSMoMVPA toolbox (32)

in combination with MATLAB 8.5 (MathWorks Natick, MA). First, a high-pass filter at 0.1 Hz

(FIR filter with transition bandwidth 0.1Hz) was applied to the continuous data. Then the data

were segmented from 1000 ms before to 1000 ms after target stimulation onset and down-

sampled to 512 Hz. Trials containing physiological or acquisition artifacts were rejected. A

semi-automatic artifact detection routine identified statistical outliers of trials and channels in

the datasets using a set of different summary statistics (variance, maximum absolute

amplitude, maximum z-value). These trials and channels were removed from each dataset.

Finally, the data were visually inspected and any remaining trials and channels with artifacts

were removed manually. Across subjects, an average of 5 channels (± 2 SD) were rejected.

Bad channels were excluded from the whole data set. A detailed report of remaining number

of trials per condition for each participant can be found in supplementary material (see Table

S2). Finally, in all further analyses and within each sensory modality for each subject, an equal

number of detected and undetected trials was randomly selected to prevent any bias across

conditions (33).

Source analyses

Neural activity evoked by stimulus onset was investigated by computing event-related

fields (ERF). For all source-level analyses, the preprocessed data was 30Hz lowpass-filtered

and projected to source-level using an LCMV beamformer analysis (34). For each participant,

realistically shaped, single-shell headmodels (35) were computed by co-registering the

participants' headshapes either with their structural MRI or – when no individual MRI was

available (3 participants and 2 participants, for the initial experiment and the control

experiment respectively) – with a standard brain from the Montreal Neurological Institute (MNI,

Montreal, Canada), warped to the individual headshape. A grid with 1.5 cm resolution based

on an MNI template brain was morphed into the brain volume of each participant. A common

spatial filter (for each grid point and each participant) was computed using the leadfields and

the common covariance matrix, taking into account the data from both conditions (detected

and undetected; or catch and sham) for each sensory modality separately. The covariance

window for the beamformer filter calculation was based on 500 ms pre- to 500 ms post-

stimulus. Using this common filter, the spatial power distribution was then estimated for each

trial separately. The resulting data were averaged relative to the stimulus onset in all

conditions (detected, undetected, catch and sham) for each sensory modality. Only for

visualization purposes a baseline correction was applied to the averaged source-level data by

subtracting a time-window from 200 ms pre-stimulus to stimulus onset. Based on a significant

difference between event-related fields of the two conditions over time for each sensory

modality, the source localization was performed restricted to specific time-windows of interest.

All source images were interpolated from the original resolution onto an inflated surface of an

MNI template brain available within the Caret software package (36). The respective MNI

coordinates and labels of localized brain regions were identified with an anatomical brain atlas

(AAL atlas; (37)) and grouped according to a network parcellation atlas (38).

Multivariate Pattern Analysis (MVPA) decoding

MVPA decoding was performed for the period 0 to 500 ms after stimulus onset based

on normalized (z-scored) single trial source data downsampled to 100Hz (i.e. time steps of 10

ms). We used multivariate pattern analysis as implemented in CoSMoMVPA (32) in order to

identify when and what kind of common network between sensory modality is activated during

the near-threshold detection task. We defined two classes for the decoding related to the task

behavioral outcome (detected and undetected). For decoding within the same sensory

modality, single trial source data were randomly assigned to one of two chunks (half of the

original data).

For decoding of all sensory modalities together, single trial source data were pseudo-

randomly assigned to one of the two chunks with half of the original data for each sensory

modality in each chunk. Data were classified using a 2-fold cross-validation procedure, where

a Bayes-Naive classifier predicted trial conditions in one chunk after training on data from the

other chunk. For decoding between different sensory modality, single trial source data of one

modality were assigned to one testing chunk and the trials from other modalities were

assigned to the training chunk. The number of target categories (e.g. detected / undetected)

was balanced in each training partition and for each sensory modality. Training and testing

partitions always contained different sets of data.

First, the temporal generalization method was used to explore the ability of each

classifier across different time points in the training set to generalize to every time point in the

testing set (21). In this analysis we used local neighborhoods features in time space (time

radius of 10ms: for each time step we included as additional features the previous and next

time sample data point). We generated temporal generalization matrices of task decoding

accuracy (detected/undetected), mapping the time at which the classifier was trained against

the time it was tested. Generalization of decoding accuracy over time was calculated for all

trials and systematically depended on a specific between or within sensory modality decoding.

The reported average accuracy of the classifier for each time point corresponds to the group

average of individual effect-size: the ability of classifiers to discriminate 'detected' from

'undetected' trials. We summarized time generalization by keeping only significant accuracy

for each sensory modalities decoding. Significant classifiers' accuracies were normalized

between 0 and 1:

$$y_t = \frac{x_t - min(x)}{max(x) - \ min(x)} \tag{1}$$

Where x is a variable of all significant decoding accuracies and x_t is a given significant

accuracy at time t. Normalized accuracies (y_t) were then averaged across significant testing

time and decoding conditions. The number of significant classifier generalization across

testing time points and the relevant averaged normalized accuracies were reported along

training time dimension (see Figure 3B). For all significant time points previously identified we

performed a 'searchlight' analysis across brain sources and time neighborhood structure. In

this analysis we used local neighborhoods features in source and time space. We used a time

radius of 10ms and a source radius of 3 cm. All significant searchlight accuracy results were

averaged over time and only the maximum 10% significant accuracy were reported on brain

maps for each sensory modality decoding condition (Figure 4).

Finally, we applied the same type of analysis to all sensory modalities by taking all

blocks together with detected and undetected NT trials (equalized within each sensory

modalities). For the control experiment, we equalized trials based on the 2x2 design with

detection report ("detected" or "undetected") and type of response ("button press = response"

or "no response"), so that we get the same number of trials inside each category (i.e. class)

for each sensory modality. We performed similar decoding analysis by using different classes

definition: either "detected vs. undetected" or "response vs. no response" (Figure 5B and C).

Statistical analysis

Detection rates for the experimental trials were statistically compared to those from the

catch and sham trials, using a dependent-samples T-Test. Concerning the MEG data, the

main statistical contrast was between trials in which participants reported a stimulus detection

and trials in which they did not (detected vs. undetected).

The evoked response at the source level was tested at the group level for each of the

sensory modalities. To eliminate polarity, statistics were computed on the absolute values of

source-level event-related responses. Based on the global average of all grid points, we first

identified relevant time periods with maximal difference between conditions (detected vs.

undetected) by performing group analysis with sequential dependent T-tests between 0 and

500 ms after stimulus onset using a sliding window of 30 ms with 10ms overlap. P-values were

corrected for multiple comparisons using Bonferroni correction. Then, in order to derive the

contributing spatial generators of this effect, the conditions 'detected' and 'undetected' were

contrasted for the specific time periods with group statistical analysis using nonparametric

cluster-based permutation tests with Monte Carlo randomization across grid points controlling

for multiple comparisons (39).

The multivariate searchlight analysis results discriminating between conditions were

tested at the group level by comparing the resulting individual accuracy maps against chance

level (50%) using a non-parametric approach implemented in CoSMoMVPA (32) adopting

10.000 permutations to generate a null distribution. P-values were set at p<0.005 for cluster

level correction to control for multiple comparisons using a threshold-free method for clustering

(40), which has been used and validated for MEG/EEG data (41, 42). The time generalization

results at the group level were thresholded using a mask with corrected z-score>2.58 (or

$p_{corrected}$<0.005) (Figure 3A). Time points exceeding this threshold were identified and reported

for each training data time course to visualize how long time generalization was significant

over testing data (Figure 3B). Significant accuracy brain maps resulting from the searchlight

analysis on previously identified time points were reported for each decoding conditions. The

maximum 10% of averaged accuracies were depicted for each significant decoding clusters

on brain maps (Figure 4).

Results

Behavior

We investigated participants' detection rate for NT, Sham and Catch trials separately

for the initial and the control experiment. During the initial experiment participants had to wait

for a response screen and press a button on each trial to report their perception (Figure 1A).

During the control experiment, however a specific response screen was used to control for

motor response mapping. At each trial the participants must use a different response mapping

related to circle's color surrounding the question mark during response screen (see Figure

1C).

For the initial experiment and across all participants (N = 16), detection rates for NT

experimental trials were: 50% (SD: 11%) for auditory runs, 56% (SD: 12%) for visual runs and

55% (SD: 8%) for tactile runs. The detection rates for the catch trials were 92% (SD: 11%) for

auditory runs, 90% (SD: 12%) for visual runs and 96% (SD: 5%) for tactile runs. The mean

false alarm rates in sham trials were 4% (SD: 4%) for auditory runs, 4% (SD: 4%) for visual

runs and 4% (SD: 7%) for tactile runs (Figure 1B). Detection rates of NT experimental trials in

all sensory modality significantly differed from those of catch trials (auditory: $T_{15} = -14.44$, p

< 0.001; visual: $T_{15} = -9.47$, p < 0.001; tactile: $T_{15} = -20.16$, p < 0.001) or sham trials (auditory:

$T_{15} = 14.66$, p < 0.001; visual: $T_{15} = 16.99$, p < 0.001; tactile: $T_{15} = 20.66$, p < 0.001).

Similar results were observed for the control experiment across all participants (N =

14), detection rates for NT experimental trials were: 52% (SD: 17%) for auditory runs, 43%

(SD: 17%) for visual runs and 42% (SD: 12%) for tactile runs. The detection rates for the catch

trials were 97% (SD: 2%) for auditory runs, 95% (SD: 5%) for visual runs and 95% (SD: 4%)

for tactile runs. The mean false alarm rates in sham trials were 11% (SD: 4%) for auditory

runs, 7% (SD: 6%) for visual runs and 7% (SD: 6%) for tactile runs (Figure 1B). Detection rates

of NT experimental trials in all sensory modality significantly differed from those of catch trials

(auditory: $T_{13} = -9.64$, p < 0.001; visual: $T_{13} = -10.78$, p < 0.001; tactile: $T_{13} = -14.75$, p < 0.001)

or sham trials (auditory: $T_{13} = 7.85$, p < 0.001; visual: $T_{13} = 6.24$, p < 0.001; tactile: $T_{13} = 9.75$,

p < 0.001). Overall such behavioral results were comparable to other studies (Leske et al.,

2015; Frey et al., 2016). Individual reaction-times and performances are reported in

supplementary materials (see Table S3).

Figure 1. Experimental designs and behavioral results. (**A-B**) Initial experiment; (**C-D**) Control experiment; (**A**) After a variable inter-trial interval between 1.3-1.8 s during which participants fixated on a central white dot, a tactile/auditory/visual stimulus (depending on the run) was presented for 50 ms at individual perceptual intensity. After 500 ms, stimulus presentation was followed by an on-screen question mark, and participants indicated their perception by pressing one of two buttons (i.e. stimulation was 'present' or 'absent') with their right hand. (**B** & **D**) The group average detection rates for NT stimulation were around 50% across the different sensory modalities. Sham trials in white (no stimulation) and Catch trials in dark (high intensity stimulation) were significantly different from the NT condition in grey within the same sensory modality for both experiments. Error bars depict the standard deviation. (**C**) Identical timing parameters were used in the control experiment; however, a specific response screen design was used to control for motor response mapping. Each trial the participants must use a different response mapping related to circle's color surrounding the question mark during response screen. Two colors (blue or yellow) were used and presented randomly during the control experiment. One color was associated to the following response mapping rule: "press the button only if there is a stimulation" (for near-threshold condition: "detected") and the other color was associated to the opposite response mapping: "press a button only if there is no stimulation" (for near-threshold condition: "undetected"). The association between one response mapping and a specific color (blue or yellow) was fixed for a single participant but was predefined randomly across different participant.

 Event-related neural activity

To compare poststimulus processing for 'detected' and 'undetected' trials, evoked

responses were calculated at the source level for the initial experiment. As a general pattern

over all sensory modalities, source-level event-related fields (ERF) averaged across all brain

sources show that stimuli reported as detected resulted in pronounced post-stimulus neuronal

activity, whereas unreported stimuli did not (Figure 2A). Similar general patterns were

observed for the control experiment with identical univariate analysis (see supplementary

Figure S2). ERFs were significantly different over the averaged time-course with specificity

dependent on the sensory modality targeted by the stimulation. Auditory stimulations reported

as detected elicit significant differences compared to undetected trials first between 190 and

210 ms, then between 250 and 425ms and finally between 460 and 500 ms after stimulus

onset (Figure 2A – left panel). Visual stimulation reported as detected elicits a large increase

of ERF amplitude compared to undetected trials from 230-250ms and from 310-500 ms after

stimulus onset (Figure 2A – middle panel). Tactile stimulation reported as detected elicits an

early increase of ERF amplitude between 95 and 150 ms then a later activation between 190

and 425 ms after stimulus onset (Figure 2A – right panel). Source localization of these specific

time periods of interest were performed for each modality (Figure 2B). The auditory condition

shows significant early source activity mainly localized to bilateral auditory cortices, superior

temporal sulcus and right inferior frontal gyrus, whereas the late significant component was

mainly localized to right temporal gyrus, bilateral precentral gyrus, left inferior and middle

frontal gyrus. A large activation can be observed for the visual conditions including primary

visual areas, fusiform and calcarine sulcus and a large fronto-parietal network activation

including bilateral inferior frontal gyrus, inferior parietal sulcus and cingulate cortex. The early

contrast of tactile evoked response shows a large difference in the brain activation including

primary and secondary somatosensory areas, but also a large involvement of right frontal

activity. The late contrast of tactile evoked response presents brain activation including left

frontal gyrus, left inferior parietal gyrus, bilateral temporal gyrus and supplementary motor

area.

Figure 2. NT trials event-related responses for different sensory modalities: auditory (left panel), tactile (middle panel) and visual (right panel). (**A**) Source-level absolute value of group event-related average (solid line) and standard error of the mean (shaded area) in the detected (red) and undetected (blue) condition for all brain sources. Significant time windows are marked with bottom solid lines (black line: $p_{Bonferroni-corrected} < 0.05$) for the contrast detected vs. undetected trials. The relative source localization maps are represented in part B for the averaged time period. (**B**) Source reconstruction of the significant time period marked in part A for the contrast detected vs. undetected trials, masked at $p_{cluster-corrected} < 0.05$.

Decoding and multivariate searchlight analysis across time and brain regions

We investigated the generalization of brain activation over time within and between the

different sensory modalities. To this end, we performed a multivariate analysis of

reconstructed brain source-level activity from the initial experiment. Time generalization

analysis presented as a time-by-time matrix between 0 and 500 ms after stimulus onset shows

significant decoding accuracy for each condition (Figure 3A). As can be seen on the black

cells located on the diagonal in Figure 3A, cross-validation decoding was performed within the

same sensory modality. However, off-diagonal red cells of Figure 3A represent decoding

analysis between different sensory modality. Inside each cell, data reported along the diagonal

(dashed line) reveal average classifiers accuracy for a specific time point used for the training

and testing procedure, whereas off-diagonal data reveal a potential classifier ability to

generalize decoding based on different training and testing time points procedure. Indeed, we

observed the ability of the same classifier trained on a specific time point to generalize its

decoding performance over several time points (see off-diagonal significant decoding inside

each cell of Figure 3A). In order to appreciate this result, we computed the average duration

of significant decoding on testing time points based on the different training time points (Figure

3B). On average, decoding within the same modality, the classifier generalization starts after

200 ms and we observed significant maximum classification accuracy after 400 ms (see Figure

3B - top panel).

Early differences specific to the tactile modality have been grasped by the classification

analysis by showing significant decoding accuracy already after 100 ms without strong time

generalization for this sensory modality, where auditory and visual conditions show only

significant decoding starting around 250-300 ms after stimulus onset. Such an early dynamic

specific to the tactile modality could explain off-diagonal accuracy for all between modalities

decoding where the tactile modality was involved (Figure 3A). Interestingly, time generalization

analysis concerning between sensory modality decoding (red cells in Figure 3A) revealed

significant maximal generalization at around 400 ms (see Figure 3B - bottom panel). In

general, the time-generalization analysis revealed time-clusters restricted to late brain activity

with maximal decoding accuracy on average after 300 ms for all conditions. The similarity of

this time-cluster over all three sensory modalities suggests the generality of such brain

activation.

Restricted to the respective significant time clusters (Figure 3A), we investigated the

underlying brain sources resulting from the searchlight analysis within and between conditions

(Figure 4). The decoding within the same sensory modality revealed higher significant

accuracy in relevant sensory cortex for each specific modality condition (see Figure 4; brain

plots on diagonal). However, decoding searchlight analysis between different sensory

modalities revealed higher decoding accuracy in fronto-parietal brain regions in addition to

diverse primary sensory regions (see Figure 4; brain plots off diagonal).

Figure 3. Time-by-time generalization analysis within and between sensory modality (for NT trials). 3x3 matrices of decoding results represented over time (from stimulation onset to 500 ms after). **(A)** Each cell presents the result of the searchlight MVPA with time-by-time generalization analysis where classifier accuracy was significantly above chance level (50%) (masked at $p_{corrected}$<0.005). For each temporal generalization matrix, a classifier was trained at a specific time sample (vertical axis: training time) and tested on all time samples (horizontal axis: testing time). The black dotted line corresponds to the diagonal of the temporal generalization matrix, i.e., a classifier trained and tested on the same time sample. This procedure was applied for each combination of sensory modality, i.e. presented on the first row is decoding analysis performed by classifiers trained on the auditory modality and tested on auditory, visual or tactile (1st, 2nd and 3rd column respectively) for the two classes: detected and undetected trials. The cells contoured with black line axes (on the diagonal) correspond to within the same sensory modality decoding, whereas the cells contoured with red line axes correspond to between different modalities decoding. **(B)** Summary of average time-generalization and decoding performance over time for all within modality analysis (top panel: average based on the 3 black cells of part A) and between modalities analysis (bottom panel: average based on the 6 red cells of part A). For each specific training time point on the x-axis the average duration of classifier's ability to significantly generalize on testing time points was computed and reported on the y-axis. Additionally, normalized average significant classifiers accuracies over all testing time for a specific training time point is represented as a color scale gradient.

Figure 4. Spatial distribution of significant searchlight MVPA decoding within and between sensory modality. Source brain maps for average decoding accuracy restricted to the related time-generalization significant time-by-time cluster (cf. Figure 3A). Brain maps were thresholded by only showing 10% maximum significant decoding accuracy for each respective time-by-time cluster. Dark solid lines separate all between sensory modality decoding brain maps from the cross-validation within one sensory modality decoding analysis on the diagonal.

Decoding and multivariate searchlight analysis over all sensory modality

We further investigated the decoding generalizability of brain activity patterns across all sensory modality in one analysis by decoding detected versus undetected trials over all blocks together (Figure 5A). We performed this specific analysis with data from the initial experiment but also with data from the control experiment in order to replicate our findings and control for potential motor response bias (see Figure 5 B and C). By delaying the response-mapping to after the stimulus presentation in a random fashion during the control experiment, neural patterns during relevant periods putatively cannot be confounded by response selection / preparation. Importantly, analysis performed on the control experiment used identical data in

figure 5B and C, but only trials assignation (i.e. 2 classes definition) for decoding was different:

"detected versus undetected" (Figure 5B) or "response versus no response" (Figure 5C).

Only decoding of conscious report (i.e. "detected versus undetected") was showing

significant time-by-time clusters where the ability for one classifier to generalize across time

seem to increase linearly after a critical time point around 300ms (Figure 5A – top panel).

Similar results were found in the control experiment (Figure 5B). However, we did not find any

significant decoding related to motor response preparation (Figure 5C), illustrating the

successful experimental control of the potential confound.

Restricted to the respective significant time clusters (Figure 5 - middle panel), we

investigated the underlying brain sources resulting from the searchlight analysis (Figure 5 –

bottom panel). Interestingly, significant brain regions of between-sensory decoding revealed

common network localization with a strikingly similar pattern over both experiments (Figure

5A and B). This result highlights a brain network that includes frontal and parietal regions,

such as inferior frontal and parietal gyrus, but also primary sensory areas related to the task,

motor regions and deep brain structure such as precuneus or hippocampus (see Table S1).

By using a parcellation atlas (38), we depicted regions belonging to different known brain

networks including sensory systems, default mode, attentional and fronto-parietal network

(43).

Figure 5. Time-by-time generalization and brain searchlight decoding analysis across all sensory modalities (for NT trials). Decoding results represented over time (from stimulation onset to 500 ms after). **(A) Initial experiment,** first row shows result of the searchlight MVPA with time-by-time generalization analysis of "detected" versus "undetected" trials across all sensory modalities. Second row shows the time-clusters where classifier accuracy was significantly above chance level (50%) (masked at $p_{corrected}$<0.005). The black dotted line corresponds to the diagonal of the temporal generalization matrix, i.e., a classifier trained and tested on the same time sample. Third row shows the spatial distribution of significant searchlight MVPA decoding between sensory modalities for the significant time clusters identified above. Brain maps were thresholded (masked at $p_{corrected}$<0.001). **(B) Control experiment**, similar analysis and plots regarding the contrast "detected" versus "undetected" by using identical number of trials with counterbalancing number of absence or presence of motor response for NT trials. **(C) Control experiment**, similar analysis and plots regarding the contrast "response" versus "no response" by using identical number of trials with counterbalancing number of detected or undetected target stimulation for NT trials.

Discussion

For a neural process to be a strong contender as a neural correlate of consciousness, it should show some generalization e.g. across sensory modalities. This has –despite being implicitly assumed- never been directly tested. To pursue this important issue, we investigated a standard NT experiment targeting three different sensory modalities in order to explore common spatio-temporal brain activity related to conscious perception using multivariate and searchlight analysis. Our findings focusing on the post-stimulus evoked responses are in line with previous studies for each specific sensory modality, showing stronger brain activation when the stimulation was reported as perceived (27, 28, 44). Importantly by exploiting the advantages of decoding, we provide for the first time direct evidence of common electrophysiological correlates of conscious access across sensory modalities.

ERF time-course differences across sensory modalities

Our first results suggest significant temporal and spatial differences when a univariate contrast between 'detected' and 'undetected' trials was used to investigate sensory-specific evoked responses. At the source level, the global group average activity revealed different significant time periods according to the sensory modality targeted where modulations of evoked responses related to detected trials can be observed (Figure 2A). In the auditory and visual modalities, we found mainly significant differences after 200 ms. In the auditory domain, perception- and attention-modulated sustained responses around 200 ms from sound onset were found in bilateral auditory and frontal regions using MEG (45, 46). Using MEG, a previous study confirmed awareness-related effects from 240 to 500 ms after target presentation during visual presentation (47).

Our results show early differences in the transient responses (for the contrast detected versus undetected) for the somatosensory domain compared to the other sensory modalities, and have been previously identified using EEG at around 100 and 200 ms (48). Moreover, previous MEG studies have shown early brain signal amplitude modulation (<200ms) related

to tactile perception in NT tasks (28, 49, 50). Such differences are less pronounced regarding

the contrast between catch and sham trials across sensory modality (Figure S1). Early ERF

difference for the tactile NT trials can be due to the experimental setup where auditory and

visual targets stimulation emerged from a background stimulation (constant white noise and

screen display) whereas tactile stimuli remain isolated transient sensory targets. Despite these

differences the time generalization analysis was able to grasp similar brain activity occurring

at different time scale across these three sensory modalities.

Source localizations performed with univariate contrasts for each sensory modality

suggest differences in network activation with some involvement of similar brain regions in late

time windows such as: inferior frontal gyrus, inferior parietal gyrus and supplementary motor

area. However, qualitatively similar topographic patterns observed in such analysis cannot

easily be interpreted as similar brain processes. The important question is whether these

neural activity patterns within a specific sensory modality can be used to decode subjective

report of the stimulation within a different sensory context. The multivariate decoding analysis

we performed in the next analysis aimed to answer this question.

Identification of common brain activity across sensory modalities

Multivariate decoding analysis was used to refine spatio-temporal similarity across

these different sensory systems. In general, stable characteristics of brain signals have been

proposed as a transient stabilization of distributed cortical networks involved in conscious

perception (51). Stability and timing differences of brain activity related to conscious

perception across sensory systems have been explored with the time generalization analysis.

The presence of similar brain activity can be revealed between modalities using such a

technique, even if significant ERF modulation is distributed over time. As expected, between-

modality time-generalization analysis involving tactile runs show off-diagonal significant

decoding due to early significant brain activity for the tactile modality (Figure 3A). This result

suggests the existence of early but similar brain activity patterns related to conscious

perception in the tactile domain compared to auditory and visual modalities.

Generally, decoding results revealed a significant time cluster starting after 300 ms

with high classifier accuracy that speaks in favor of a late neural response related to conscious

report. Actually, we observed the ability of the same classifier trained on specific time points

with a specific sensory modality condition to generalize its decoding performance over several

time points with the same or another sensory modality. This result speaks in favor of

supramodal brain activity patterns that are consistent and stable over time. In addition, the

searchlight analysis across brain regions highlighted a common brain network activation

during these significant time-generalization clusters. Note that, as seen also in multiple other

studies using decoding (22, 23, 42, 52), the average accuracy can be relatively low and yet

remains significant at the group level. Note however that contrary to many other cognitive

neuroscientific studies using decoding (52, 53), we do not apply the practice of "subaveraging"

trials to create "pseudo"-single trials, which naturally boosts average decoding accuracy (54).

Also, the statistical rigor of our approach is underlined by the facts that the reported decoding

results are restricted to highly significant effects (at least $P_{corrected}<0.005$; see Methods section).

Critically, we replicated our results -applying the identical very conservative statistical

thresholds- within a second control experiment when looking at conscious perception report

contrast independently from motor response activity (Figure 5).

Our results conform to those of previous studies in underlying the importance of late

activity patterns as crucial markers of conscious access (7, 55) and decision-making

processes (10, 56). In this study, we extend the involvement of a parieto-frontal network across

three different sensory systems. Some of the brain regions found in our searchlight analysis,

namely the superior frontal cortex and inferior parietal cortex, are shared with other functional

brain networks such as the salience network (57, 58). These regions have been previously

found to be activated by attention-demanding cognitive tasks (59).

Hence, we would like to emphasize that one cannot conclude from our study that the

observed supramodal network is exclusively devoted to conscious report. Brain networks

identified in this study share common brain regions and dynamics with the attentional and

salience networks that remain relevant mechanisms to performing a NT-task. Moreover, some

brain regions involved in motor planning were identified with our analysis, such as

supplementary motor area or precentral gyrus, and could in principle relate to the upcoming

button-press to report the subjective perception of the stimulus. However, we specifically

targeted such motor preparation bias within the control experiment, in which the participant

was unable to predict a priori how to report a conscious percept (i.e. pressing or withholding

a button press) until the response prompt appeared. Importantly, we did not found any

significant decoding when trials used for the analysis where sorted under response type (e.g.

with or without an actual button press from the participant) compared to subjective report of

detection (see Figure 5B and C). In contrast, we replicated our previous results with strikingly

similar findings with smaller significant decoding extends in time and space compared to the

initial experiment regarding conscious perception report (i.e. "detected versus undetected")

(see Figure 5A and B). The control experiment, due to its design, was more difficult for the

participants compared to the initial one because response mapping was randomly chosen at

each trial. Such experimental context potentially added noise to the trial-by-trial subjective

perceptual report. Overall, this specific design with our conservative statistical choices and a

smaller sample size could explain smaller significant time and brain regions clusters extends

in our last analysis (Figure 5B) compared to the initial experiment (Figure 5A).

Late involvement of all primary sensory cortices

Interestingly, our analysis revealed that primary sensory regions are strongly involved

in decoding conscious perception across sensory modalities. This important result suggests

that sensory cortices from a specific modality contain sufficient information to allow the

decoding perceptual conscious access in another different sensory modality. In line with the

idea of the broadcasting of an integrated conscious percept (7), these results suggest a late

active role of primary cortices over three different sensory systems (Figure 5). One study

reported efficient decoding of visual object categories in early somatosensory cortex using

fMRI and multivariate pattern analysis (60). Another fMRI experiment suggested that sensory

cortices appear to be modulated via a common supramodal frontoparietal network, attesting

to the generality of attentional mechanism toward expected auditory, tactile and visual

information (61). However, in our study we demonstrate how local brain activity from different

sensory regions reveal a specific dynamic allowing generalization over time to decode the

behavioral outcome of a subjective perception in another sensory modality. These results

speak in favor of intimate cross-modal interactions between modalities in perception (62).

Finally, our results suggest that primary sensory regions remain important at late

latency after stimulus onset for resolving stimulus perception over different sensory modalities.

We propose that this network could enhance the processing of behaviorally relevant signals,

here the sensory targets. Although the integration of classically unimodal primary sensory

cortices into a processing hierarchy of sensory information is well established (63), some

studies suggest multisensory roles of primary cortical areas (64, 65).

Today it remains unknown how such multisensory responses could be related to an

individual's unisensory conscious percepts in human. Since sensory modalities are usually

interwoven in real life, our findings of a supramodal network that may subserve both conscious

access and attentional functions have a higher ecological validity than results from previous

studies on conscious perception for single sensory modality.

Actually, our results are in line with an ongoing debate in neuroscience asking to which

extend multisensory integration emerges already in primary sensory areas (65, 66). Animal

studies provided compelling evidence suggesting that the neocortex is essentially

multisensory (67). Here our findings speak in favor of a multisensory interaction in primary and

associative cortices. Interestingly a previous an fMRI study by using multivariate decoding

revealed distinct mechanisms governing audiovisual integrations in primary and associative

cortices needed for spatial orienting and interactions in a multisensory world (68).

Conclusion

We successfully characterized common patterns over time and space suggesting

generalization of consciousness-related brain activity across different sensory NT tasks. To

our knowledge, this is the first study to report significant spatio-temporal decoding across

different sensory modalities in a near-threshold perception experiment. Indeed, our results

speak in favor of the existence of stable and supramodal brain activity patterns, distributed

over time and involving seemingly task-unrelated primary sensory cortices. The stability of

brain activity patterns over different sensory modalities presented in this study is, to date, the

most direct evidence of a common network activation leading to conscious access (2).

Moreover, our findings add to recent remarkable demonstrations of applying decoding and

time generalization methods to MEG (21–23, 69), and show a promising application of MVPA

techniques to source level searchlight analysis with a focus on the temporal dynamics of

conscious perception.

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Author contributions

674   G.S. and N.W. conceived the approach. G.S. and T.H. implemented the experiment. G.S. and

675   M.F. collected the data. G.S. analyzed the data. G.S. and N.W. wrote the manuscript. All

676   authors approved the current manuscript.

Resource sharing and data availability

679   Further information and requests for resources or data should be directed to and will be fulfilled

680   by the corresponding author.

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