

# An Efficient Moments-Based Inference Method for Within-Host Bacterial Infection Dynamics

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## Abstract

1  
2 Over the last ten years, isogenic tagging (IT) has revolutionised the study of bacterial  
3 infection dynamics in laboratory animal models. However, quantitative analysis of IT  
4 data has been hindered by the piecemeal development of relevant statistical models. The  
5 most promising approach relies on stochastic Markovian models of bacterial population  
6 dynamics within and among organs. Here we present an efficient numerical method to fit  
7 such stochastic dynamic models to *in vivo* experimental IT data. A common approach  
8 to statistical inference with stochastic dynamic models relies on producing large numbers  
9 of simulations, but this remains a slow and inefficient method for all but simple prob-  
10 lems, especially when tracking bacteria in multiple locations simultaneously. Instead, we  
11 derive and solve the systems of ordinary differential equations for the two lower-order mo-  
12 ments of the stochastic variables (mean, variance and covariance). For any given model  
13 structure, and assuming linear dynamic rates, we demonstrate how the model parameters  
14 can be efficiently and accurately estimated by divergence minimisation. We then apply  
15 our method to an experimental dataset and compare the estimates and goodness-of-fit to  
16 those obtained by maximum likelihood estimation. This flexible framework can easily be  
17 applied to a range of experimental systems. Its computational efficiency paves the way  
18 for model comparison and optimal experimental design.

19                    **Author Summary:**

20                    Recent advancements in technology have meant that microbiologists are producing vast  
21                    amounts of experimental data. However, statistical methods by which we can analyse that  
22                    data, draw informative inference, and test relevant hypotheses, are much needed. Here,  
23                    we present a new, efficient inference tool for estimating parameters of stochastic models,  
24                    with a particular focus on models of within-host bacterial dynamics. The method relies  
25                    on matching the two lower-order moments of the experimental data (i.e., mean, variance  
26                    and covariance), to the moments from the mathematical model. The method is verified,  
27                    and particular choices justified, through a number of simulation studies. We then use this  
28                    method to estimate models that have been previously estimated using a “gold-standard”  
29                    maximum likelihood procedure.

30 **List of symbols:**

- 31 •  $A$ : number of animals
- 32 •  $T$ : number of tagged strains
- 33 •  $n$ : number of organs
- 34 •  $N_i$ : number of bacteria in organ  $i$
- 35 •  $m_{ij}$ : migration rate from organ  $i$  to organ  $j$
- 36 •  $k_i$ : killing rate in organ  $i$
- 37 •  $r_i$ : replication rate in organ  $i$
- 38 •  $\tau_i$ : observation time  $i$
- 39 •  $\mathbf{A}, \mathbf{B}, \mathbf{C}$ : matrices
- 40 •  $\boldsymbol{\lambda}$ : vector of transition rates
- 41 •  $B$ : Number of bootstrap samples
- 42 •  $\boldsymbol{\theta}^*$ : MDE parameter estimate

43 **Abbreviations:**

- 44 • ABC: approximate Bayesian computation
- 45 • IT: isogenic tagging
- 46 • LV: live vaccine
- 47 • MARE: mean absolute relative error
- 48 • MDE: minimum divergence estimate
- 49 • MLE: maximum likelihood estimate
- 50 • qPCR: quantitative polymerase chain reaction
- 51 • WITS: wildtype isogenic tagged strain

# 1 Introduction

The elucidation of basic kinetic rates governing bacterial growth during infection (such as division and death rates) has been recognised as an important challenge for over 60 years [1]. Thanks to recent technological developments in microbiology, and pushed by growing concern over antimicrobial resistance and the need for new vaccines, the last decade has witnessed rapid progress in the quantification of *in vivo* dynamics of bacterial infection in animal models. Two experimental approaches in particular have shown great promise across multiple pathogen species: isogenic tagging, the focus of this report, and fluorescence dilution, a term encompassing several techniques from which bacterial replication can be inferred [2]. Isogenic tagging (IT) consists in generating an arbitrary number of sub-clones of a given bacterial strain, each defined by a unique genetic tag (a predetermined nucleotide sequence) inserted in a non-coding region of the chromosome. When grown together *in vitro* or *in vivo*, every tagged strain behaves identically to the original strain. Their relative frequencies within a bacterial culture can be measured by quantitative qPCR or sequencing of the tagged region. Taken together with the absolute number of viable bacteria (e.g., by plating colonies), changes in the frequencies of the tags within the bacterial population can reveal underlying variations in the rates at which bacteria divide, die and disperse. For example, a constant number of viable bacteria accompanied by a loss of some of the tags in a closed population would indicate that a certain proportion of bacteria have died and been replaced by replication. Likewise, when monitoring tag frequencies in two or more anatomical compartments within animals, a gradual homogenisation among organs can reveal the transfer of bacteria. While some studies have stopped at qualitative interpretations of such empirical patterns [3, 4, 5, 6], it is possible to quantify underlying processes with the help of mathematical models. Two different types have been used: stochastic population dynamic models to estimate bacterial division, death and migration rates [7, 8, 9, 10, 11, 12], and population genetic models to estimate bottleneck sizes [13, 14]. Our aim is to develop efficient inference methods to deal with the former type of models.

Stochastic birth–death–migration models (a canonical class of Markovian processes [15]) are a common choice to analyse IT experiments, and naturally lead to likelihood–based

82 inference, using either maximum likelihood [9, 11] or Bayesian estimation [12]. In a given  
83 experiment, assuming that all of the  $A$  animals sampled at a given time and in given condi-  
84 tions are identical, and that all of the  $T$  tagged strains infecting each animal act indepen-  
85 dently of each other and are governed by identical rates, we can treat the  $A \times T$  observed  
86 strain abundances as independent realisations of a stochastic birth–death–migration pro-  
87 cess, and calculate the likelihood of any model of interest accordingly. In most published  
88 IT studies, bacteria can grow at different rates in different locations within an animal,  
89 and migrate from one location to another, generating a network of subpopulations (or  
90 metapopulation). This increases the dimensions of both the state variable space (as the  
91 model must keep track of the multivariate distribution of bacterial abundance) and the pa-  
92 rameter space. Calculating the likelihood of such a model given an experimental dataset  
93 requires solving a complex stochastic model, which will rarely be possible analytically.  
94 Even a linear birth–death process with a non–Poisson immigration process (representing  
95 the transfer of a finite inoculum dose) is sufficient to prevent a fully analytical treat-  
96 ment, and results in a computationally intensive estimation process [12]. Alternatively,  
97 approximate–likelihood (e.g., iterative filtering [16]) or likelihood–free (e.g., approximate  
98 Bayesian computation or ABC [17]) methods involve the generation of a large number  
99 of stochastic simulations of the model of interest, which can be equally time–consuming,  
100 even when taking advantage of parallel computation. Although this may not be a problem  
101 when fitting a single model to a single dataset, it limits our ability to compare multiple  
102 models across complex datasets (typically involving multiple experimental treatments)  
103 and, beyond that, use these inference tools for the purpose of optimising experimental  
104 design [18]. Hence, there is a need for alternative inference methods using suitable ap-  
105 proximations to achieve greater gains in computational efficiency.

106 The dynamics of multivariate Markovian processes can be approximated using moment–  
107 closure methods [19]. Mathematically, a system of differential equations for the mo-  
108 ments of the state variables can be derived analytically from the governing equation of  
109 any stochastic model [20]. By effectively ignoring the higher moments, a closed, small-  
110 dimension system can be derived, allowing fast numerical solution of the lower moments at  
111 any time point. Parameter estimation can then be achieved by fitting the first and second

112 order moments of the model to the mean, variance and covariance of the corresponding  
113 variables in the data. Apart from a few proof-of-principle studies using simulated chem-  
114 ical reaction data [21, 22, 23] that show great promise, application to statistical inference  
115 from biological data remain scarce. As a rare example, Buchholz et al. [24] implemented  
116 a moment-based method to solve a multiple T-cell differentiation pathway problem, fit-  
117 ting the moments of a large number of alternative stochastic models to experimental  
118 data using a  $\chi^2$  statistic. This suggests that efficient moment-based inference methods  
119 should be made more readily available to unleash the full potential of stochastic models  
120 in experimental biology.

121 Our objective is to provide a functional and flexible computational framework to esti-  
122 mate the parameters of stochastic metapopulation models for the within-host dynamics  
123 of infection, and demonstrate its application and value to analyse IT studies. The model  
124 tracks the probability distribution of the number of copies of a tagged strain of bacteria  
125 across a network of anatomical compartments within an animal. The goal is to estimate  
126 the bacterial division and death rates within each organ, and migration rates between  
127 each pair of compartments. First, we present an algorithm that evaluates the first- and  
128 second-order moments of the state variables for arbitrary network structures, and assess  
129 its accuracy and speed against a gold standard for stochastic models: the exact Gillespie  
130 algorithm. We then compare the accuracy of several inference options against simulated  
131 data, and finally apply the most promising method to a recent dataset on the dynamics  
132 of *Salmonella enterica* serovar Typhimurium in the blood, liver and spleen of vaccinated  
133 mice [11]. The massive gain in speed compared to likelihood-based inference allows us  
134 to use parametric bootstrap to quantify parameter uncertainty and goodness-of-fit. We  
135 also demonstrate how empirically derived noise terms (e.g., caused by imprecise data  
136 collection) can be taken into account.

## 2 Methodology

### 2.1 Biological context

We consider the general case of a bacterial pathogen inoculated into an animal host where it can potentially reach  $n$  anatomical compartments—which can be distinct organs, tissues, lumens, or predefined sections thereof. All our examples are motivated by IT experiments in which a set of identical animals receive the same initial inoculum dose in one compartment (e.g., mouth, nose, blood, peritoneum, etc) at time  $t = 0$ . The inoculum is composed of an even mix of  $T$  tagged strains. At given times  $\tau_1, \tau_2$  etc, a subset of  $A_1, A_2$ , etc animals are chosen at random and euthanised. The abundance of each tagged strain in each of the  $n$  anatomical compartments of interest is measured. Thus, at a given time  $\tau_i$ , the data consist of a matrix  $\mathbf{D}_i$  with  $n$  rows by  $A_i T$  columns, filled with observed bacterial numbers. From this matrix, we can calculate the observed moments, namely the mean and variance of strain abundance within each compartment, and the covariance between each pair of compartments.

Depending on the experimental procedures, these observations are usually subject to some degree of uncertainty, due to observational error. In general we assume that this error is random with a mean of zero, so that there is no systematic bias; this should be assessed by the researchers who conducted the experiments. As a result, we assume that the observed means are unbiased, but the observed (co)variances may be incorrect. In Section 2.7, we describe how known sources of error can be accounted for as part of the data processing procedure. In addition, there usually is some uncertainty about the actual inoculum dose received by each animal. Variations in the abundance of each strain should be assessed experimentally by testing several inoculum doses: this provides estimates for the initial mean and variance of the number of bacteria present in the target compartment at  $t = 0$ .

We emphasise a few key assumptions and caveats of the present study, which we review in further detail in the Discussion. First, the variable of interest from a modelling perspective is the abundance of a single tagged strain, rather than the total bacterial load per animal (as the latter can be obtained by adding up individual strains). Indeed,

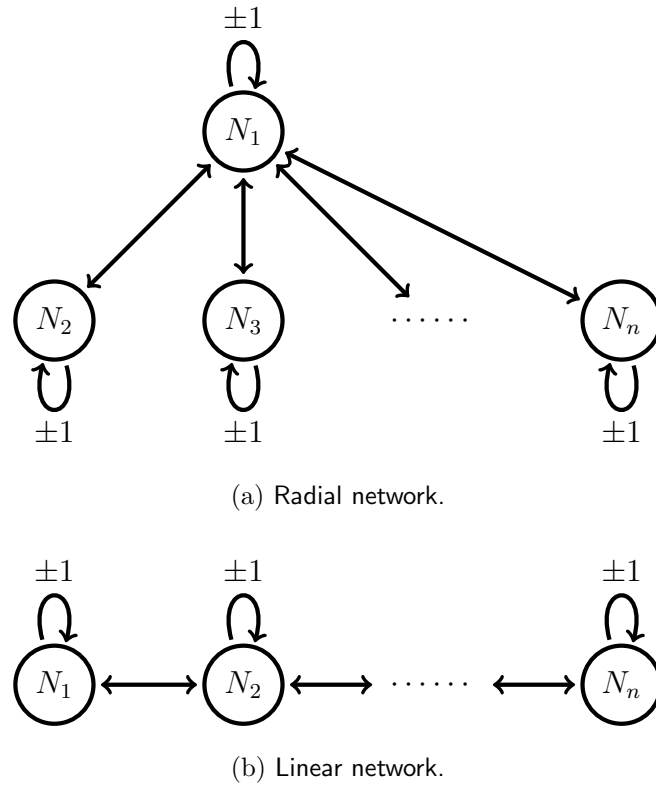


166 our model framework assumes that, over the time period considered and for a given set  
167 of initial conditions, the rates of bacterial division, death and migration *per capita* are  
168 independent of the total bacterial load. Second, we assume that all the bacterial cells are  
169 governed by identical probabilities of division, death and migration. While this excludes  
170 the case of so-called persister cells (i.e., a subset of bacteria with a much lower division  
171 rate than the rest) or similar discrete partition, it is worth noting that the stochastic model  
172 we describe below does generate continuous variations in the times of events, consistent  
173 with empirical distributions of bacterial replication in vivo [25].

## 174 2.2 Stochastic model framework

175 As a function of time  $t$  since inoculation, the vector of positive integer state variables  
176  $\mathbf{N}(t) = \{N_1(t), \dots, N_n(t)\}$  represents the simultaneous abundance of bacteria in com-  
177 partments 1 to  $n$ . In the context of IT studies, this represents a single tagged strain.  
178 Three types of stochastic events drive the bacterial dynamics: division (which adds one  
179 bacterium to a given compartment), death (which removes one bacterium from a given  
180 compartment) and migration (which moves one bacterium from one compartment to an-  
181 other). Assuming linear transition rates, we have a total of  $n$  division rates  $r_i N_i$  and  
182 death rates  $k_i N_i$  within organ  $i$ , and  $n(n - 1)$  migration rates  $m_{i,j} N_i$  from compartment  
183  $i$  to  $j$ . Note that specific models may assume that some of the parameters are equal to  
184 zero, for example if there is no physical connection between given pairs of compartments.

185 In particular, we consider two geometries, illustrated in Figure 1, corresponding to two  
186 typical anatomical topologies of relevance to bacterial infection: a radial network with a  
187 central compartment (e.g., bloodstream supplying every organ), and a linear network  
188 (e.g., digestive track).



**Figure 1:** Diagram illustrating the two types of network structure we consider.

### 2.3 Computation of the first- and second-order moments

The method we propose for parameter inference relies on the first two moments of the stochastic system. That is, we use only the expected number of bacteria within each compartment, the variance of the number of bacteria within each compartment, and the pair-wise covariances. A simple approach to generating these moments for a particular stochastic system in terms of the model parameters, is given by [26]. Letting  $\lambda = \{r_1 N_1, \dots, r_n N_n, k_1 N_1, \dots, k_n N_n, m_{1,2} N_1, \dots\}$  be the vector of transition rates, we can write the  $h^{th}$  non-central moment of the state of the  $i^{th}$  compartment as:

$$\frac{\partial}{\partial t} \mathbb{E} [N_i^h(t)] = \mathbb{E} \left[ \sum_j \lambda_j(t) [\phi_j(N_i(t))^h - N_i(t)^h] \right], \quad (1)$$

where  $\phi_j$  is a function describing the change of the state for the  $j^{th}$  transition. In Supplementary Materials (S1.7), we show that this leads to a closed, linear system of differential equations for the first moments. Letting  $\mathbf{M}_1(t) = \{\mathbb{E}[N_i(t)], 1 \leq i \leq n\}$  be the vector of first moments as a function of time, we can express these differential equations in matrix

201 form as:

$$\frac{\partial}{\partial t} \mathbf{M}_1(t) = \mathbf{A} \times \mathbf{M}_1(t), \quad (2)$$

202 which leads to the solution,

$$\mathbf{M}_1(t) = \exp(\mathbf{A}t) \times \mathbf{M}_1(0), \quad (3)$$

203 where  $\mathbf{M}_1(0)$  are the initial conditions of the system,  $\mathbf{A}$  is a time-independent matrix  
204 containing the model parameters, and  $\exp$  is the matrix exponential function.

205 Next, let  $\mathbf{M}_2(t) = \{\mathbb{E}[N_i(t)N_j(t)], 1 \leq i \leq n, 1 \leq j \leq n\}$  be the vector of second  
206 moments. By applying Duhamel's formula to the differential equations obtained from  
207 equation (1), we obtain the following expression for the second-order moments:

$$\mathbf{M}_2(t) = \exp(\mathbf{C}t) \times \mathbf{M}_2(0) + \exp(\mathbf{C}t) \times \left[ \int_0^t \exp(-\mathbf{C}s) \times \mathbf{B} \times \exp(\mathbf{A}s) ds \right] \mathbf{M}_1(0), \quad (4)$$

208 where  $\mathbf{B}$  and  $\mathbf{C}$  are time-independent matrices containing model parameters, and  $\mathbf{M}_1(0)$   
209 and  $\mathbf{M}_2(0)$  are vectors containing the initial moments. Using the numerical method for  
210 matrix exponential in [27], we can evaluate the first- and second-order moments at any  
211 time point. Remarkably, no moment-closure approach is required as the expressions for  
212 the second-order moments are independent of higher-order moments. See Supplementary  
213 Information for a full derivation.

## 214 2.4 Parameter Inference by Divergence Minimisation

215 Given a dataset consisting of one or more matrices  $\mathbf{D}$  of bacterial counts (as per section  
216 2.1), and a stochastic model (as per section 2.2), we now describe methods to estimate  
217 the parameter values of the model that minimise the divergence between the predicted  
218 and observed distributions of bacterial abundance, using only the lower moments of those  
219 distributions. Specifically, we evaluate the means, variances and covariances of the  $N_i$   
220 variables at a given time  $t$ . From the corresponding matrix  $\mathbf{D}$ , we calculate the vector  
221 of observed means  $\boldsymbol{\mu}^{(\mathbf{D})}$  and the matrix of observed variance-covariance  $\mathbf{V}^{(\mathbf{D})}$ ; and from  
222 the model's solution given a set of parameters  $\boldsymbol{\theta}$ , we compute the vector of predicted  
223 means  $\boldsymbol{\mu}^{(\boldsymbol{\theta})}$  and the matrix of predicted variances-covariances  $\mathbf{V}^{(\boldsymbol{\theta})}$  which can be derived  
224 from  $\mathbf{M}_2(t)$ . We compared four common divergence measures: a Chi-Squared metric, the  
225 Mahalanobis distance, the Hellinger distance, and the Kullback-Leibler divergence.

226 Note that none of the measures below is designed to deal with the particular situation  
 227 when any of the organs is reported void of bacteria (i.e.,  $N_i = 0$ ) in all replicates at a given  
 228 time point, i.e. if all the observed moments related to that organ are equal to zero. In  
 229 some experimental systems, this may occur as an artefact of the observation method, e.g.,  
 230 when only a small sample is measured: in this case, it is possible to “correct” the data for  
 231 sampling biases (see Section 2.7). Otherwise, a simple solution would be to remove the  
 232 moments relative to that organ from the inference procedure. In some cases, it may make  
 233 sense to completely remove the empty organ from the model if no meaningful inference  
 234 can be expected from its inclusion, as illustrated in Section 3.3.

235 The Chi-Squared metric adds up the squared pairwise-differences between each pre-  
 236 dicted moment and its corresponding observed moment, each term being scaled by the  
 237 magnitude of the observed moment. As a result, all moments are effectively treated  
 238 equally. The expression for this divergence is:

$$\Delta_{\chi} = \sum_i \frac{(\boldsymbol{\mu}_i^{(\theta)} - \boldsymbol{\mu}_i^{(D)})^2}{|\boldsymbol{\mu}_i^{(D)}|} + \sum_{i,j} \frac{(\mathbf{V}_{i,j}^{(\theta)} - \mathbf{V}_{i,j}^{(D)})^2}{\mathbf{V}_{i,j}^{(D)}} \quad (5)$$

239 The other three divergence expressions we tested make use of the fact that our chosen  
 240 statistics  $\boldsymbol{\mu}$  and  $\mathbf{V}$  are moments of distributions. Since we do not establish complete char-  
 241 acterisations of the distributions, we decided to borrow the expressions of well-known di-  
 242 vergences measures for multivariate normal distributions, as these only require the knowl-  
 243 edge of their first and second-order moments. In other words, we compute the divergence  
 244 between two multivariate normal distributions with respective moments  $(\boldsymbol{\mu}^{(D)}, \mathbf{V}^{(D)})$  and  
 245  $(\boldsymbol{\mu}^{(\theta)}, \mathbf{V}^{(\theta)})$ .

246 The Mahalanobis distance is measured between each point in the observed data, and  
 247 the distribution described by the predicted moments. That is, by estimating the param-  
 248 eters we are trying to find the distribution that these data are most likely to have been  
 249 sampled from. Specifically, each observation  $\mathbf{X}_j$  is given by column  $j$  of the data matrix  
 250  $\mathbf{D}$ . The divergence is obtained by summing the distances to the predicted distribution  
 251 from every observation:

$$\Delta_M = \sum_j \sqrt{(\mathbf{X}_j - \boldsymbol{\mu}^{(\theta)})^T \mathbf{V}^{(\theta)^{-1}} (\mathbf{X}_j - \boldsymbol{\mu}^{(\theta)})} \quad (6)$$

252 The squared Hellinger distance is given by:

$$\Delta_H^2 = 1 - \exp\left(-\frac{1}{8} \boldsymbol{\mu}^T \mathbf{V}^{-1} \boldsymbol{\mu} - \frac{1}{2} \log \frac{|\mathbf{V}|}{\sqrt{|\mathbf{V}^{(\theta)}| |\mathbf{V}^{(\mathbf{D})}|}}\right), \quad (7)$$

253 where  $\boldsymbol{\mu} = \boldsymbol{\mu}^{(\theta)} - \boldsymbol{\mu}^{(\mathbf{D})}$  and  $\mathbf{V} = \frac{\mathbf{V}^{(\theta)} + \mathbf{V}^{(\mathbf{D})}}{2}$ .

254 The Kullback-Leibler divergence from the predicted distribution to the observed one  
255 is given by:

$$\Delta_K = \frac{1}{2} \left[ \text{tr}(\mathbf{V}^{(\mathbf{D})^{-1}} \mathbf{V}^{(\theta)}) - n + \boldsymbol{\mu}^T \mathbf{V}^{(\mathbf{D})^{-1}} \boldsymbol{\mu} + \log \frac{|\mathbf{V}^{(\mathbf{D})}|}{|\mathbf{V}^{(\theta)}|} \right], \quad (8)$$

256 where  $\text{tr}(\cdot)$  is the trace operator. The derivations of the Hellinger and Kullback-Leibler  
257 divergences are given in Supplementary Materials S1.2.

258 Even though these expressions may not provide correct estimates of the actual “Ma-  
259 halanobis distance”, “Hellinger distance” and “Kullback-Leibler divergence” between the  
260 data and the predicted distributions (as these are not normally distributed), they still pro-  
261 vide adequate divergence measures: they all return positive values which are only equal  
262 to zero (hence are minimised) when  $\boldsymbol{\mu}^{(\theta)} = \boldsymbol{\mu}^{(\mathbf{D})}$  and  $\mathbf{V}^{(\theta)} = \mathbf{V}^{(\mathbf{D})}$ , which occurs when  
263 the data are drawn from the predicted distribution. We use that property for the purpose  
264 of parameter inference, given a dataset and a model. The set of parameter values  $\boldsymbol{\theta}$  that  
265 minimises the divergence measure is termed the “minimum divergence estimate” (MDE).

266 All code was written in R [28]. We used the `UObyQA` optimisation routine in the `powell`  
267 package [29].

## 268 2.5 Bootstrap Variance Estimate

269 In order to quantify the uncertainty in our parameter estimates conditional on the dynamic  
270 model considered, we utilise the parametric bootstrap method (e.g., [30]), which can  
271 be exploited simply here due to the computational efficiency of the inference approach.  
272 Having obtained an MDE,  $\boldsymbol{\theta}^*$  for a given data matrix  $\mathbf{D}$  and a given model, we simulate  
273  $B$  data sets from the model at these parameters (i.e.,  $\mathbf{x}^b \sim f(x | \boldsymbol{\theta}^*)$ ,  $b = 1, \dots, B$ ). For  
274 each simulation, we estimate the corresponding parameters using the MDE technique ( $\boldsymbol{\theta}^b$ ,  
275  $b = 1, \dots, B$ ). These  $B$  estimated parameters are used to estimate the variance-covariance  
276 matrix of the parameter estimates. Subsequently, one can use this matrix to estimate

277 confidence intervals in a number of ways [31]. For simplicity, the analysis in Section 3.3  
278 uses the `ellipse` package in R [32] to obtain approximate 95% confidence intervals of  
279 the model parameters (that is, assuming the bootstrapped parameter estimates follow a  
280 multivariate normal distribution).

## 281 **2.6 Model Goodness-of-fit**

282 In order to assess the model goodness-of-fit, we once again utilise the parametric boot-  
283 strap. Concurrent to calculating the uncertainty estimates using the MDE method, the  
284 divergences corresponding to each simulated data set at their estimated parameter val-  
285 ues are recorded. These bootstrapped divergences can thus be used to represent the null  
286 distribution of divergences for the model at the estimated parameter values – giving a  
287 representation of the divergences we should expect from the model at these values. The  
288 divergence estimated for the observed data is then compared to the null distribution to  
289 obtain a p-value for the hypothesis that the data could have been generated by the model.

## 290 **2.7 Data analysis with observational noise**

291 A common source of error when fitting a model to experimental data is the observation  
292 process. In the type of microbiology experiments considered here, where the data represent  
293 bacterial loads in infected animals, there are at least two steps that affect the accuracy  
294 of the measurements: sampling (when only part of the bacterial loads are recovered) and  
295 and quantitation (the process by which the number of bacterial cells in the samples is  
296 measured). For example, in a recent IT experiment [11], sampling error was modelled  
297 as a binomial process (as known fractions of each homogenised organ were plated) and  
298 quantitation error was modelled using a log-normal distribution which was estimated  
299 empirically using an independent control experiment (in which known numbers of bacterial  
300 colonies were processed by qPCR in the same way as bacterial samples extracted from  
301 animals in the main experiment). Although both error distributions were centred on the  
302 true bacterial numbers (i.e. the mean numbers of bacteria were not biased), the variance  
303 and covariance in the reported data would not have been accurate estimates of the variance  
304 and covariance within the animals: hence our MDE could be biased if we did not account

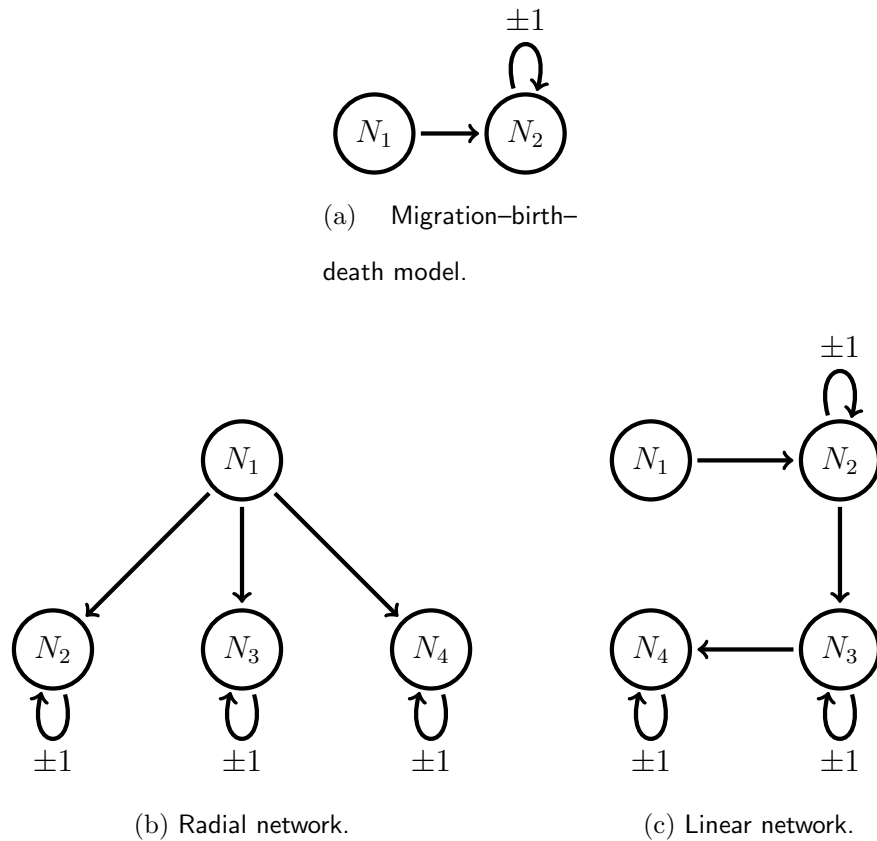
305 for observational errors.

306 In our present reanalysis of those data, we integrate both error terms before perform-  
307 ing parameter inference, using the following procedure. Our goal is to propose a simple  
308 heuristic which could be applied to any experimental dataset with known (or assumed)  
309 observational error distributions. First, we generate a large number of stochastic simula-  
310 tions of the model under a biologically reasonable range of parameter values (i.e. using  
311 uniform prior distributions across sensible ranges) to generate “perfect” observations. We  
312 then calculate the corresponding “perfect moments” from every simulated dataset. Next,  
313 we apply the observation noise to the simulated data, and calculate the corresponding  
314 “observed moments”. We then use linear regression models to establish a relationship  
315 between each of the perfect and observed moments (with transformations where appro-  
316 priate), with weights given by the simulations proximity to the actual observed moments  
317 from the experiment. This calibrated regression model is then applied to the moments  
318 of the experimental data of interest, in order to estimate the moments of the true, unob-  
319 served bacterial loads in the animals. We eventually compute MDE using these corrected  
320 moments.

321 We note that for some models of the observation process, it may be possible to establish  
322 analytic relationships between the “perfect” and “observed” moments using conditional  
323 expectation and variance theory (e.g., [33]). The choice of suitable correction methods  
324 for a given system will depend on both the model complexity and the level of empirical  
325 quantification of observation noise.

### 326 **3 Results**

327 We begin by demonstrating the speed and accuracy of the computation of the first- and  
328 second-order moments for arbitrary network structures, compared to Gillespie simula-  
329 tions. We then assess the four previously mentioned divergence measures to validate our  
330 minimum divergence estimation procedure with each model, across a range of parameter  
331 values. Finally, we apply our inference method to reanalyse a published experimental  
332 dataset, and compare the results with the previous maximum likelihood estimates.



**Figure 2:** Illustrations of three representative model structures.

### 3.1 Moment computation

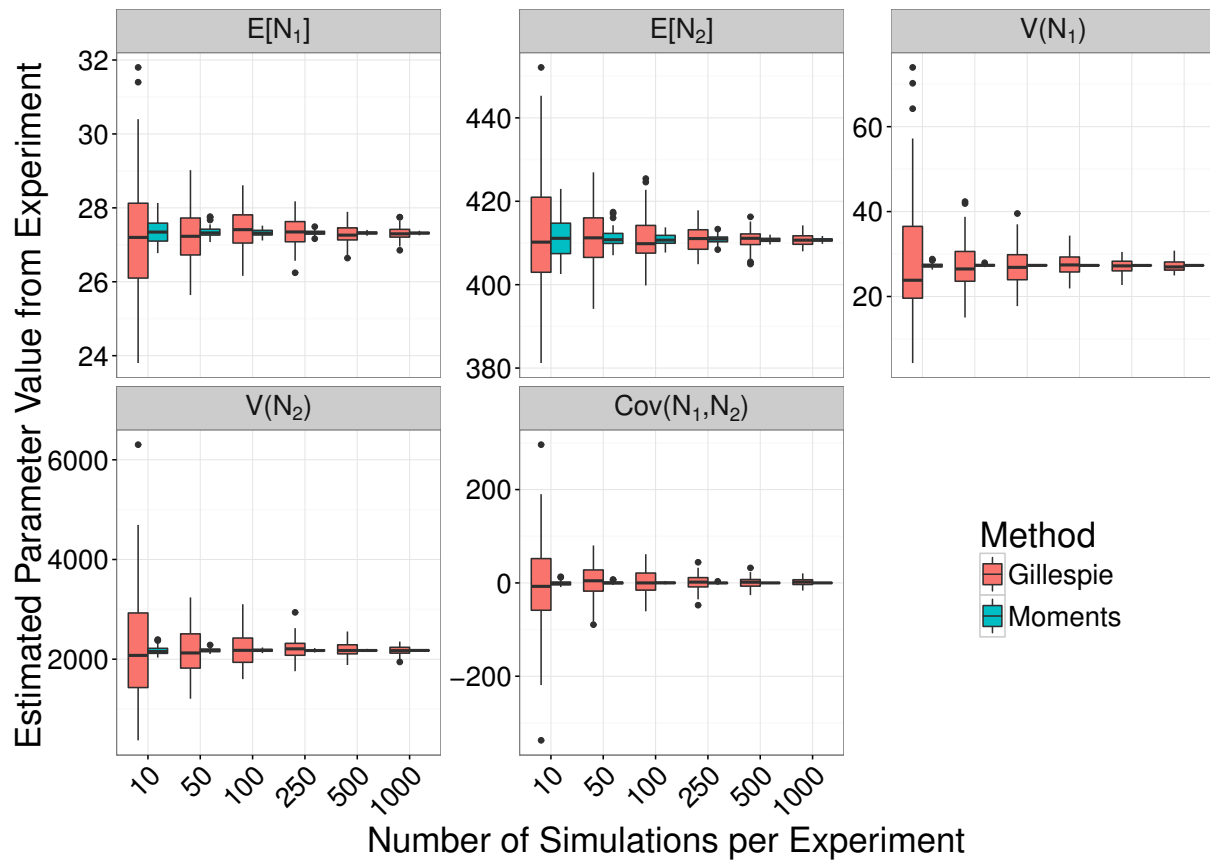
As a proof-of-concept, we compare our proposed computation method of the means, variances and covariances of bacterial loads, with the values derived from large numbers of Gillespie simulations, across a range of model structures and parameter values. Our results illustrate the computational effort required to obtain the same level of accuracy with each method. For each model and each parameter set, we simulated 100 experiments, each consisting of 10, 50, 100, 250, 500, or 1000 observations (representing the product of the number of animals  $A$  by the number of tagged strains  $T$  as per section 2.1) at a given time, without observational error. The initial bacterial loads at  $t = 0$  in each replicate experiment were drawn at random from a Poisson distribution, to mimic typical variability in inoculum doses in experiments [11]. We considered three model structures, illustrated in Fig. 2: (a) basic migration-birth-death model, (b) four-compartment radial network, and (c) four-compartment linear network. For each virtual experiment, we calculated the



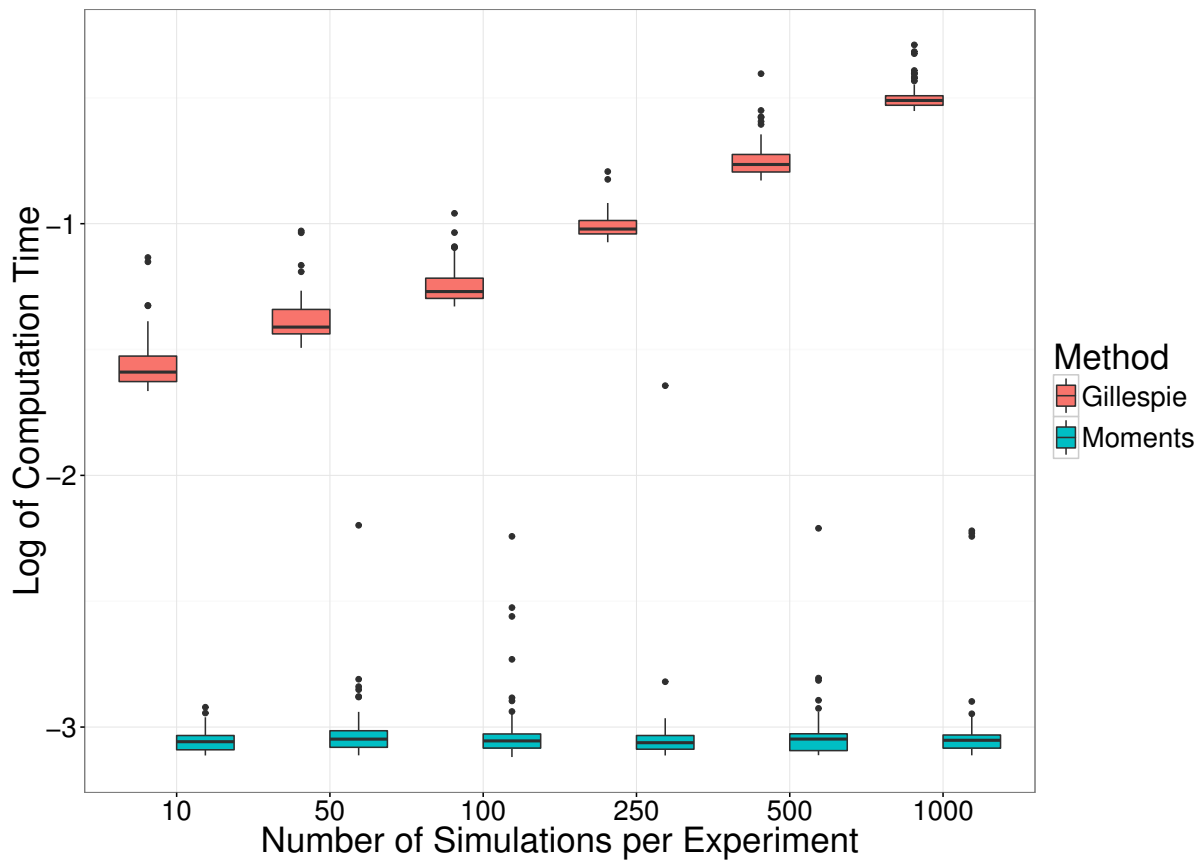
346 first- and second-order moments of the bacterial loads in two ways at a given time point  
347 ( $t = 6$  for the basic migration-birth-death model, and  $t = 4$  for the four-compartment  
348 radial and linear network).

349 We randomly drew the stated number of initial conditions (ranging from 10 to 1000),  
350 and evaluated the moments at the future time point in the following two ways. First,  
351 we used Gillespie simulations to progress each initial condition forward to the stated  
352 observation time, and then calculated the moments from the collection of simulations.  
353 Second, we took the stated number of initial conditions to estimate the moments at time  
354 zero, and used these to evaluate the moments at the observation time using equations (3)  
355 and (4); we refer to this as the direct moment-calculation method.

356 Figure 3 shows that there is still a greater amount of variation in the moments from  
357 1000 Gillespie simulations, compared to the direct approach. The direct method pro-  
358 duces less variable moment estimates as experiment size increases, as a result of more  
359 accurate estimates of the initial distribution of bacteria. Furthermore, the computation  
360 time of the Gillespie approach increases steadily with the number of simulations, while  
361 the direct method is consistently more efficient, independent of the size of the experiment  
362 (Figure 4). Similar patterns are shown in the Supplementary Materials (S1.3) for the  
363 four-compartment linear and radial network models.



**Figure 3:** Box plots of estimated moments from 100 simulated experiments using the two-compartment birth-death-migration model (Figure 2a). For each experiment (of size 10, 50, 100, 250, 500 or 1000), the lower moments of variables  $N_1$  and  $N_2$  at time  $t = 6$  were calculated from Gillespie simulations (red boxes) or from the moments equations ("direct method", blue boxes), starting from Poisson-distributed initial conditions. The stated number of simulations per experiments is equivalent to the total number of replicate observation ( $A_i T$  at time point  $\tau_i$  as per section 2.1).



**Figure 4:** Box plots of computation time to evaluate the moments from 100 simulated experiments of the two-compartment birth-death-migration model, as per Figure 3. The vertical axis shows the logarithm in base 10 of running times in seconds.

### 3.2 Divergence Measures: Simulation Study

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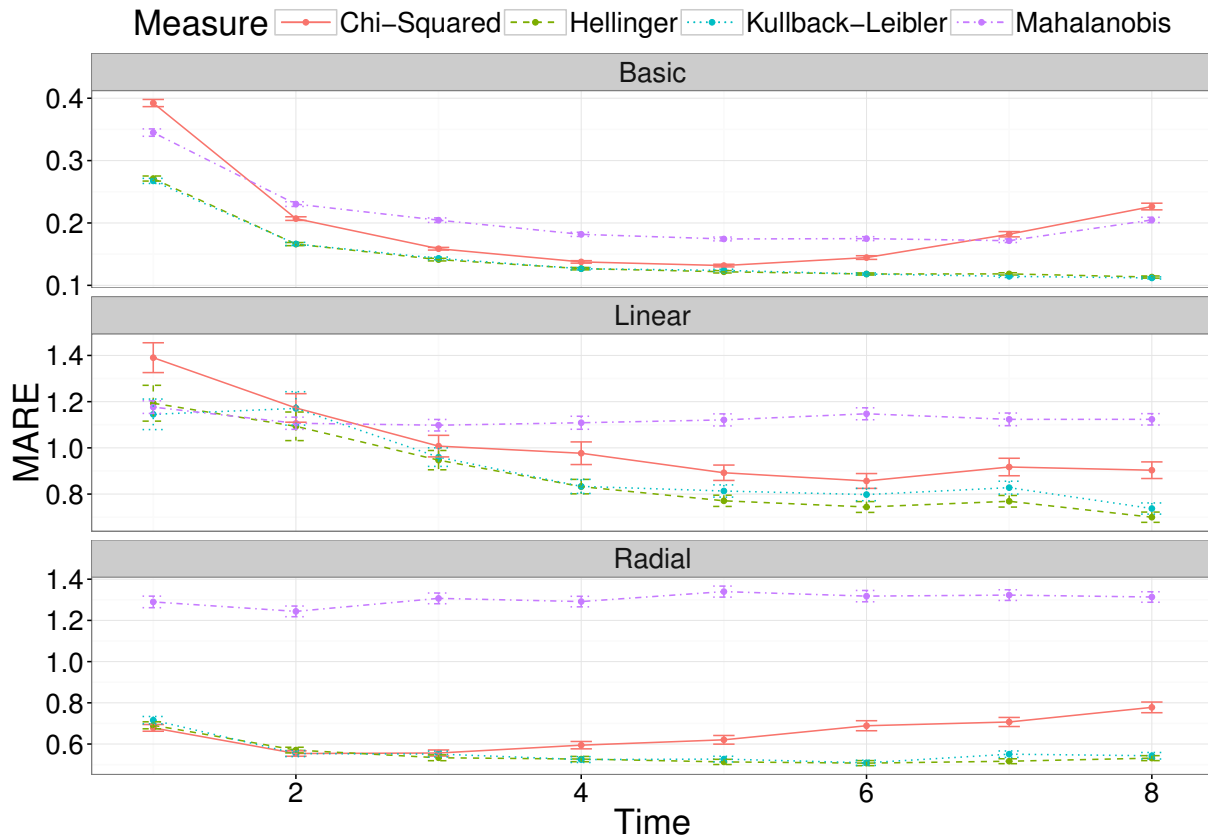
Next, we compare the accuracy of MDE among the four candidate divergence measures, using data simulated from the same three model structures as in the previous section and across a range of parameter values. For each model structure and each parameter combination, we ran 100 series of 100 Gillespie simulations from  $t = 0$  to each of 8 observation times, representing 800 experiments (each of size 100) with “perfect” observations of the system (i.e., without experimental noise). This process was repeated for a set of different parameter values for each model to represent different scenarios – three representative values for each parameter in the basic model ( $3^3 = 27$  scenarios), and five randomly generated sets of parameters for the four compartment linear and radial networks with parameters. The initial conditions for each simulation, in every scenario, were randomly

375 generated from a Poisson distribution with mean parameter 200. The optimisation rou-  
376 tine was initiated at randomly generated conditions each time, with each parameter values  
377 drawn independently from a Uniform(0,1) distribution.

378 From the results of each simulated experiment, we computed the MDE using each of the  
379 Chi-Squared, Mahalanobis, Hellinger, and Kullback-Leibler divergences. The performance  
380 of each divergence was measured by the mean absolute relative error (MARE). That  
381 is, under scenario  $s$ , with  $p$  target parameters  $\theta_s = (\theta_{1s}, \theta_{2s}, \dots, \theta_{ps})$ , and estimated  
382 parameters  $\hat{\theta}_{sj} = (\hat{\theta}_{1sj}, \hat{\theta}_{2sj}, \dots, \hat{\theta}_{psj})$  for the  $j^{th}$  simulation, the MARE is given by:

$$\text{MARE}_{s,j} = \frac{1}{p} \sum_{i=1}^p \frac{|\theta_{is} - \hat{\theta}_{isj}|}{\theta_{is}}$$

383 Figure 5 displays the average error across each scenario for the four divergence mea-  
384 sures, at a range of observation times, for each of the three models under consideration.  
385 We can see that both the Hellinger and Kullback-Leibler divergence measures perform  
386 considerably better than the Chi-Squared and Mahalanobis divergences for the Basic,  
387 Linear and Radial networks. The similar performance of the Hellinger and Kullback-  
388 Leibler divergences is not unexpected, due to their relationship. We observe a marginal  
389 advantage in favour of the Kullback-Leibler divergence for the basic and radial network,  
390 and thus we use the Kullback-Leibler divergence in analysing experimental data in Sec-  
391 tion 3.3. The results aggregated by scenario for each model are shown in Supplementary  
392 Materials S1.4.

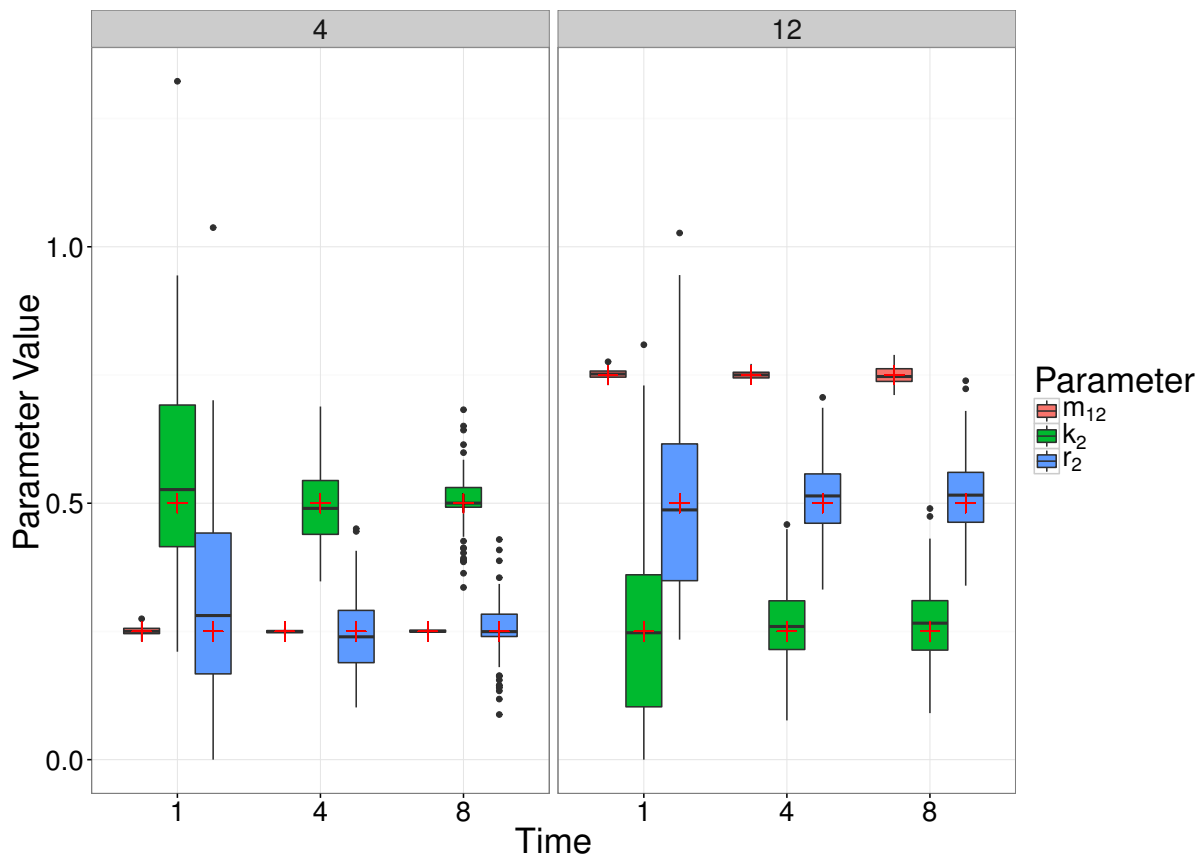


**Figure 5:** The average mean absolute relative error (MARE) across a number of observation times, for the two-compartment network (top panel), the linear four-compartment network (middle panel) and the radial four-compartment network (bottom panel). Each point is the average for that measure, at that observation time, with error bars representing the standard error.

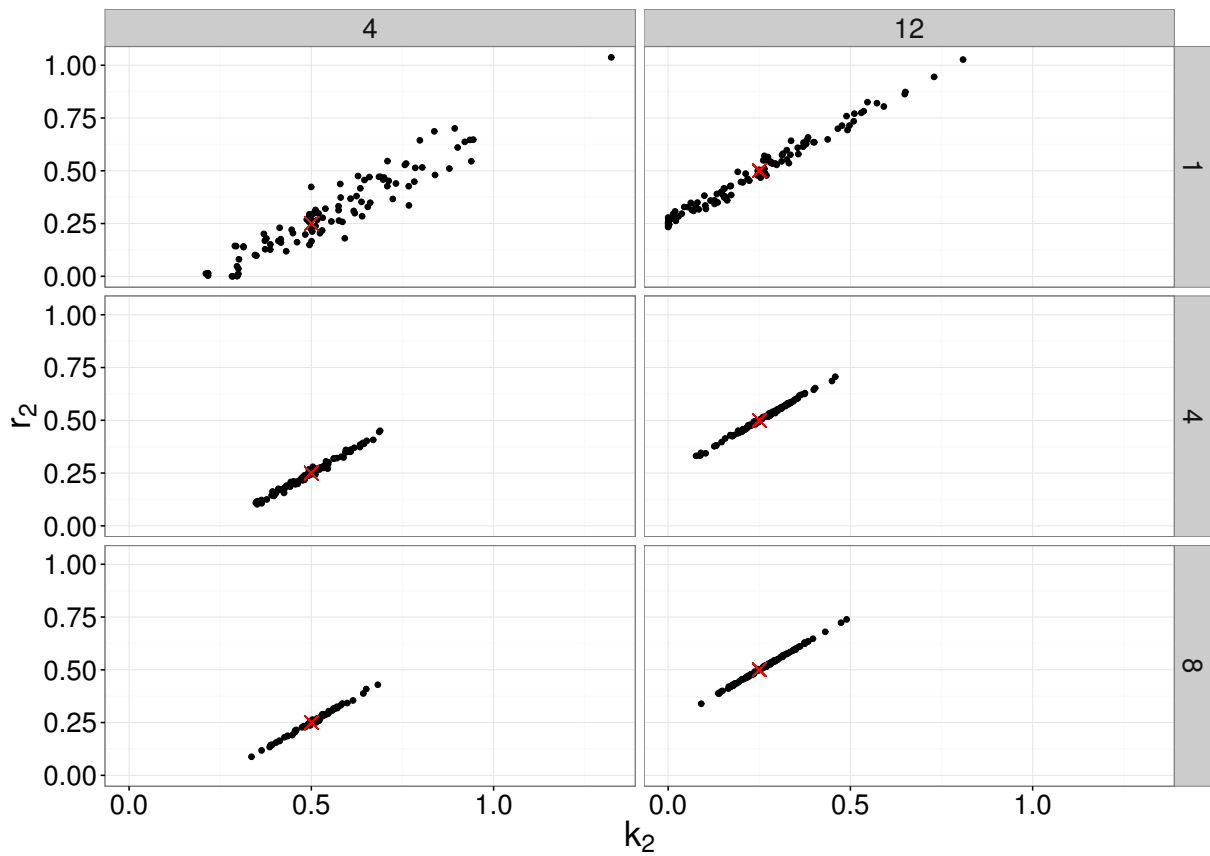
393 Figure 9 further illustrates the distribution of parameter estimates for a few selected  
 394 scenarios and time points. For each time point, the variation was generated by the stochas-  
 395 tic birth-death-migration process, demonstrating the level of uncertainty in parameter  
 396 estimates due to the biological process itself. In this case, each simulated experiment was  
 397 made up of 100 simulations; fewer replicates would increase the parameter uncertainty.  
 398 At each time point, the estimates of the migration rate  $m_{12}$  are much less variable than  
 399 those of the killing rate  $k_2$  and replication rate  $r_2$ : this is actually caused by a very strong  
 400 positive correlation between the latter two parameters (Figure 7).

401 This can be understood intuitively, as the net growth rate  $r_2 - k_2$  is the main deter-  
 402 minant of the mean bacterial load in compartment 2. We also remark that the earlier

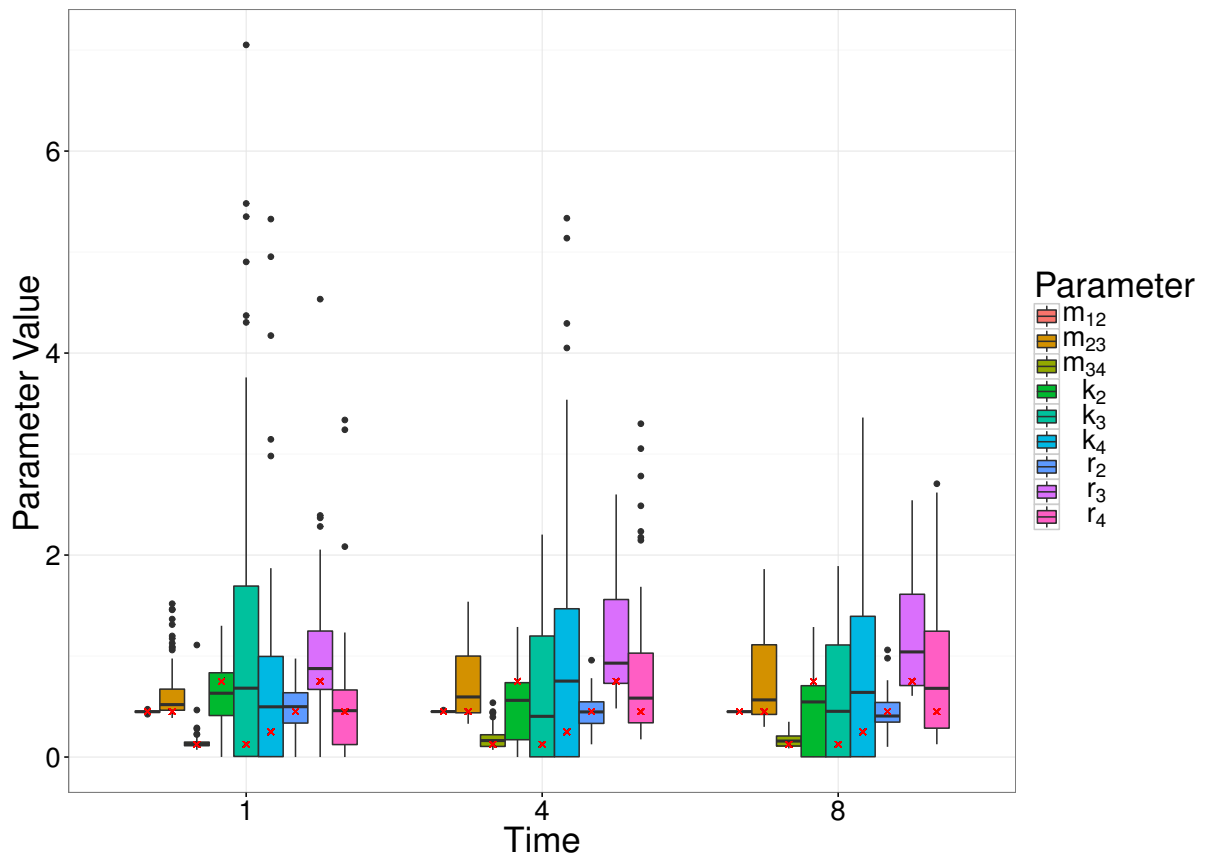
403 observation time contains more information about the clearance rate, whereas the later  
404 observation time better captures the replication and killing rates. Results of all scenarios  
405 are shown in Supplementary Materials S1.6.



**Figure 6:** Box plots of MDE's corresponding to simulated data for two different choices of parameter values (Scenario 4 and 12), at a number of different observation times (1, 4 and 8) of the simple model. The box plots represent 100 parameter estimates corresponding to the 100 simulations, and the red crosses denote the true parameter value.

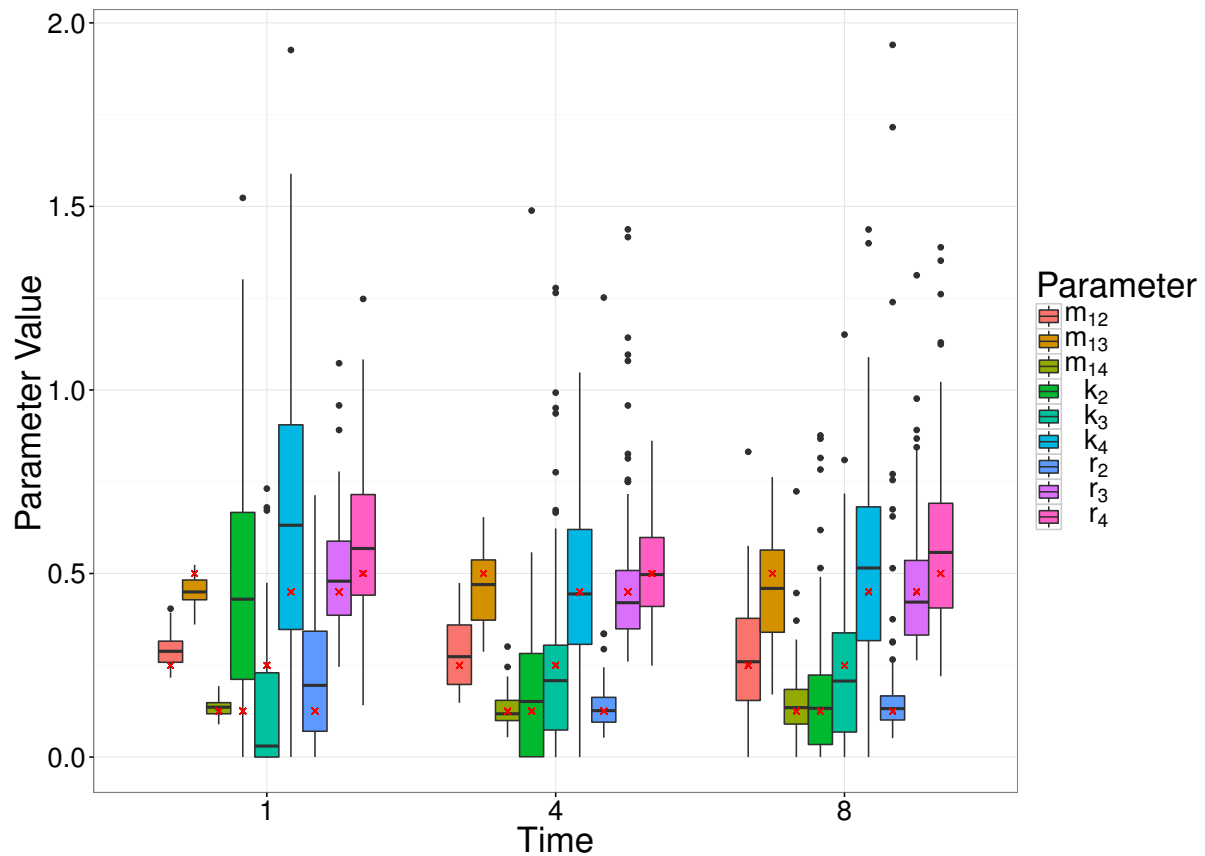


**Figure 7:** Bivariate plot of MDE's corresponding to simulated data for two different choices of parameter values (Scenario 4 and 12), at a number of different observation times (1, 4 and 8) of the simple model. The points represent 100 parameter estimates of  $r_2$  and  $k_2$  corresponding to the 100 simulations, and the red crosses denote the true parameter value.



**Figure 8:** Box plots of MDE's corresponding to simulated data for a random set of parameter values (Scenario 4), at a number of different observation times (1, 4 and 8) of the linear model. The box plots represent 100 parameter estimates corresponding to the 100 simulations, and the red crosses denote the true parameter value.





**Figure 9:** Box plots of MDE's corresponding to simulated data for a random set of parameter values (Scenario 4), at a number of different observation times (1, 4 and 8) of the radial model. The box plots represent 100 parameter estimates corresponding to the 100 simulations, and the red crosses denote the true parameter value.

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### 3.3 Analysis of experimental data

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#### 3.3.1 Description of the system

Finally, we performed a re-analysis of experimental data from [11], in which groups of mice received an intravenous dose of *Salmonella enterica* Typhimurium, composed of an even mixture of 8 wildtype isogenic tagged strains (WITS). Bacterial loads and WITS composition were measured in the blood, liver and spleen of 10 mice at each observation time. During the first phase of the WITS experiments (represented by the first two time points at 0.5 and 6 hours post inoculation), the only biologically relevant processes considered are: migration of bacteria from blood to liver or spleen, replication and death

inside the liver and the spleen. That is, on state space  $\mathcal{S} = \{(n_B, n_L, n_S) \mid n_B, n_L, n_S \geq 0\}$ , we have the following transition rates:

$$\begin{aligned} q_{(n_B, n_L, n_S), (n_B-1, n_L+1, n_S)} &= c_L n_L, & q_{(n_B, n_L, n_S), (n_B-1, n_L, n_S+1)} &= c_S n_S, \\ q_{(n_B, n_L, n_S), (n_B, n_L+1, n_S)} &= r_L n_L, & q_{(n_B, n_L, n_S), (n_B, n_L, n_S+1)} &= r_S n_S, \\ q_{(n_B, n_L, n_S), (n_B, n_L-1, n_S)} &= k_L n_L, & q_{(n_B, n_L, n_S), (n_B, n_L, n_S-1)} &= k_S n_S, \end{aligned}$$

where  $c_L, c_S$  are the clearance (=migration) rates from the blood into the liver and spleen respectively,  $r_L, r_S$  are the replication rates in the liver and spleen respectively, and  $k_L, k_S$  are the killing rates in the liver and spleen, respectively.

One purpose of the study in [11] was to compare the effects of two vaccines on the dynamics of infection. Here, we re-analyse two of the experimental groups: an untreated group (naive) who received no vaccine, and a group who received a live-attenuated vaccine (LV). In the naive group, in addition to the clearance, replication and killing rates, we estimated the effective inoculum size  $i_0 = N_B(0)$  to account for the possibility that some of the inoculated bacteria failed to initiate an infection process [11]. In the vaccinated group, no bacteria were recovered from the blood at either of the two observation times, hence we were unable to estimate the corresponding migration rates. Instead we assumed that the transfer of bacteria to the organs was effectively instantaneous, and sought to estimate the effective initial loads in the liver and spleen (i.e.,  $i_L = N_L(0)$  and  $i_S = N_S(0)$ ), as well as the replication and killing rates. In each case, the inoculum size is assumed to be Poisson distributed.

### 3.3.2 Parameter estimation with observation noise

We applied the MDE method to estimate the parameters corresponding to these systems, and compared the results to the estimates obtained via the MLE approach, presented in [11]. Having obtained the MDE parameter estimates, we used the bootstrap approach to calculate uncertainty intervals on the estimates, and assess the model goodness-of-fit.

As described in [11], the recorded data were subject to observation noise. In particular, only a fraction of some organs were sampled (e.g., as we are not able to fully recover the total amount of blood from an individual mouse), and there was noise introduced via the qPCR. The observed moments were adjusted using the simulation-

432 based, pre-processing procedure described in Section 2.7: we assumed that the form  
433 of the sampling was binomial, and the qPCR noise has been previously modelled us-  
434 ing a log-Normal distribution [11]. For example, for the naive group, we sampled 10,000  
435 parameters  $(c_L, c_S, k_L, k_S, r_L, r_S)$  each independently from  $U[0, 3]$ , and initial inoculum  
436  $i_0 \sim \text{Poisson}(30.33)$  (the mean WITS population calculated from plating experiments  
437 [11]). “Perfect moments” were calculated from simulations of the same size as the ex-  
438 perimental data. The corresponding observed moments were then calculated by applying  
439 the observation noise model – binomial sampling to represent the fractional sampling of  
440 organs within each mouse, and log-Normal noise to represent the qPCR noise – to each  
441 simulation, and calculating the moments. The variances were log-transformed for the pur-  
442 pose of the regression models to predict the corresponding perfect moments from those  
443 observed from the experiment.

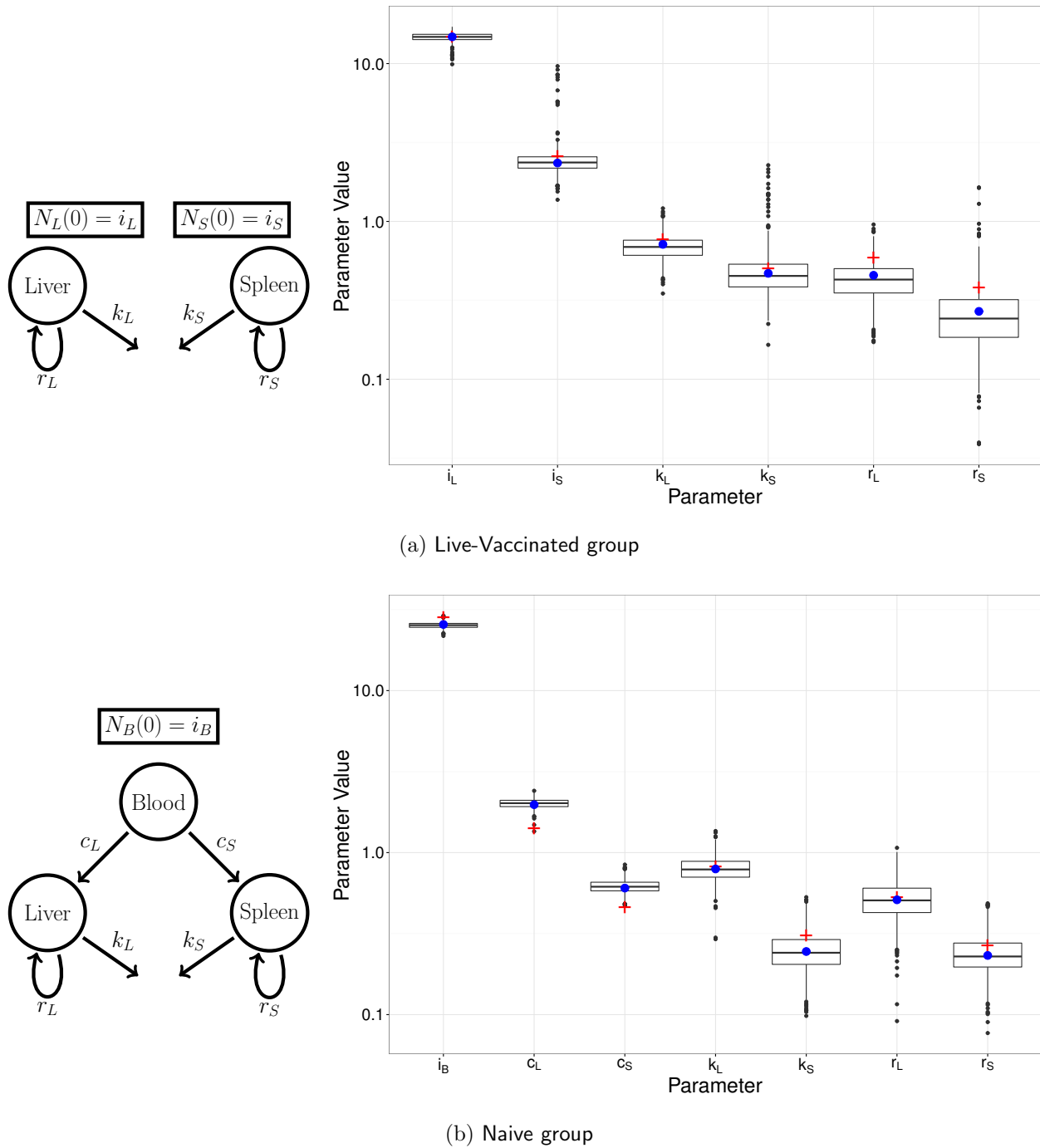
444 Figure 10 provides a comparison of the MLE and MDE estimation procedures for the  
445 naive and LV experimental groups. The box plots represent the bootstrapped parameter  
446 estimates, with the MDE parameter estimate (blue dots), and MLE parameter estimates  
447 (red crosses).

448 As explained in the previous section, the strong positive correlation between the repli-  
449 cation and killing rates within each organ, clearly visible on Figure 11, is characteristic of  
450 this system.

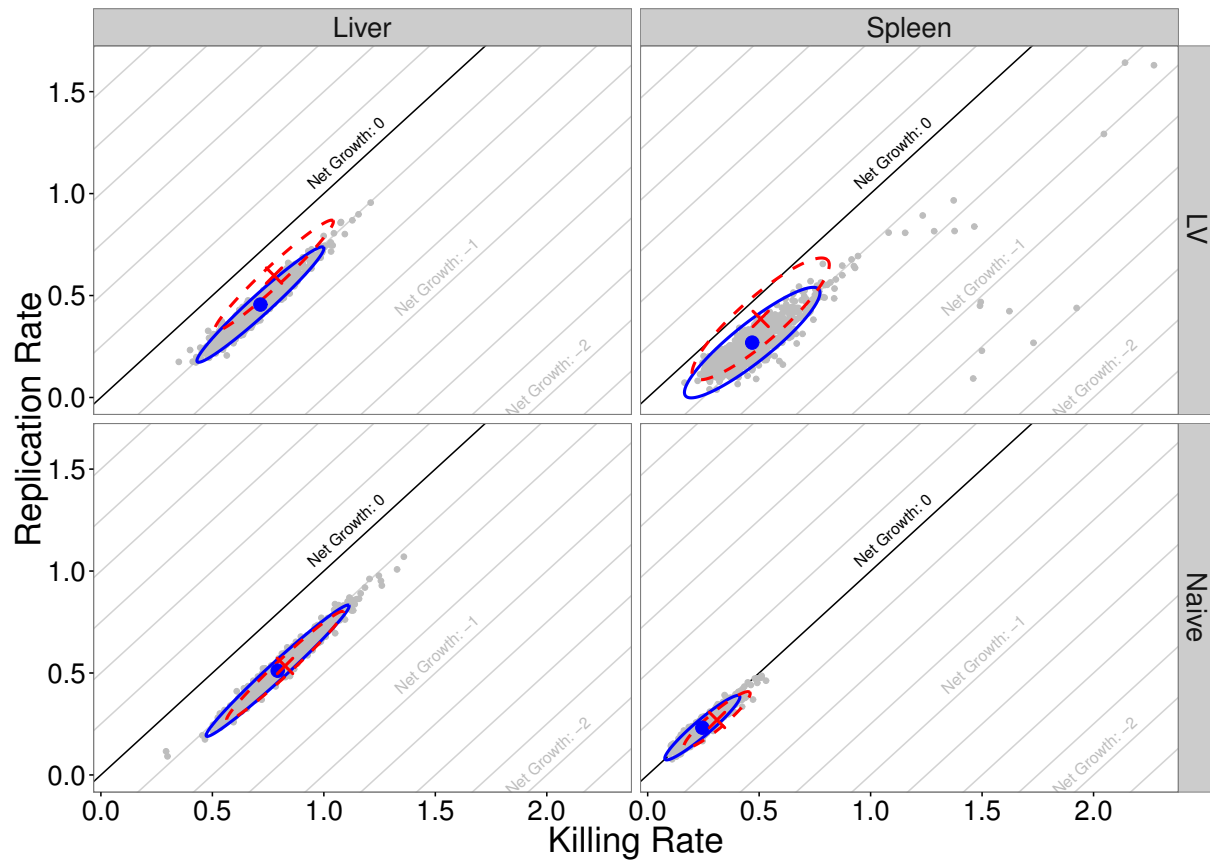
### 451 3.3.3 Model goodness-of-fit

452 In calculating the MDE parameter estimates for the bootstrap samples, we evaluated  
453 divergence measures for datasets simulated from the model. Thus, the collection of these  
454 divergences provide a suitable representation of the null distribution of divergences under  
455 this model. We compared the divergence for our observed data set to this null distribution  
456 in order to assess the model goodness-of-fit. Figure 12 demonstrates the goodness-of-fit  
457 measure for the models fit to the two experimental groups.

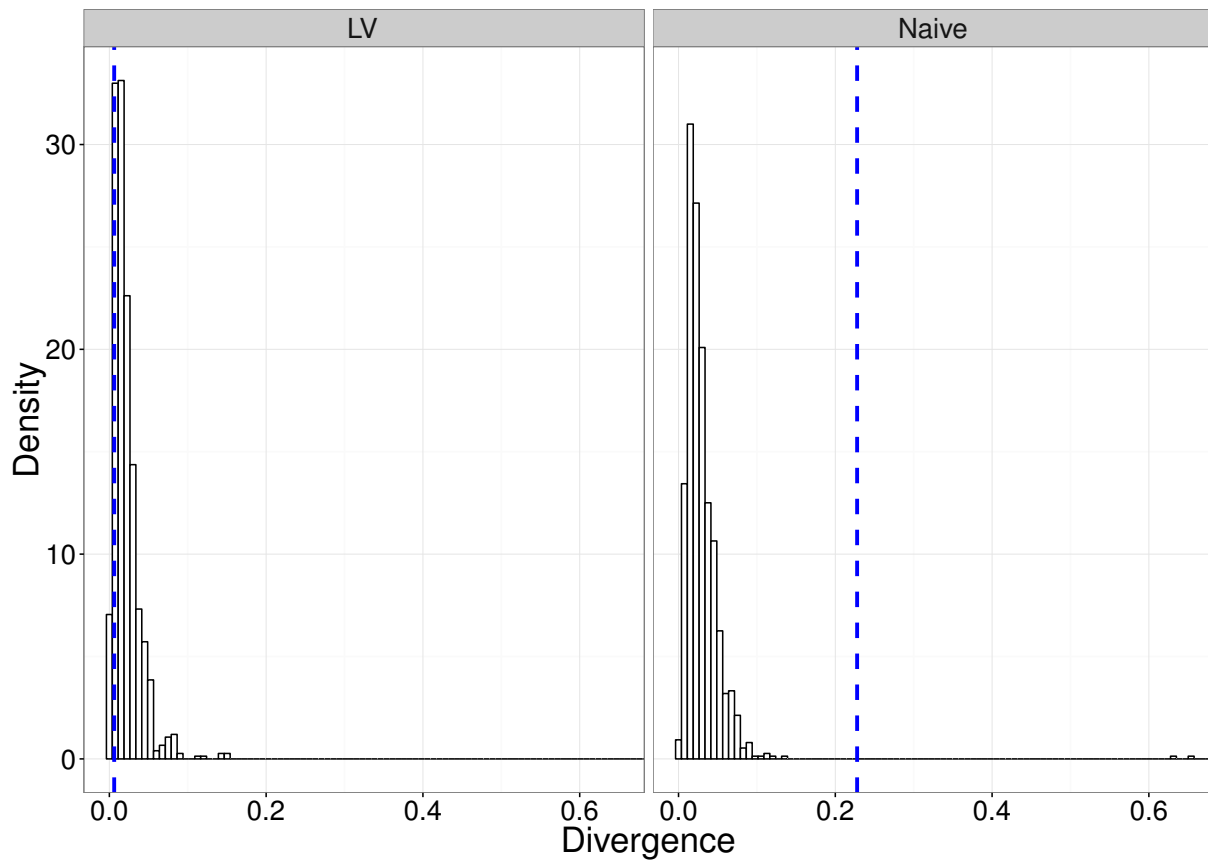
458 The approximate p-values associated with the goodness-of-fit tests for the naive and  
459 LV experimental groups are 0.002 and 0.882, respectively. This suggests that the model  
460 provides a suitable fit to the vaccinated experimental group; however, there is a non-



**Figure 10:** Left: Diagram of each model illustrating the relevant compartments, initial conditions, and rates of interest. Right: MDE parameter estimate (blue dot), MLE parameter estimate (red cross), and box plots of the bootstrapped parameter estimates.



**Figure 11:** Bivariate distributions of replication and killing rates in liver and spleen, for both naive and live-vaccinated groups. Blue circles are the MDE values, with the blue (solid) ellipses representing the 95% confidence ellipses calculated using the 1000 bootstrap samples (grey points). The red crosses are the MLE values, with red (dashed) ellipse calculated using the hessian evaluated at the MLE.



**Figure 12:** Figures demonstrating the goodness-of-fit of the two models to the respective data sets. The histogram bars are the bootstrapped estimate of the null distribution of divergences under the model at the estimated parameter values for the respective model. The (blue) vertical dashed-line is the divergence corresponding to the observed data set.

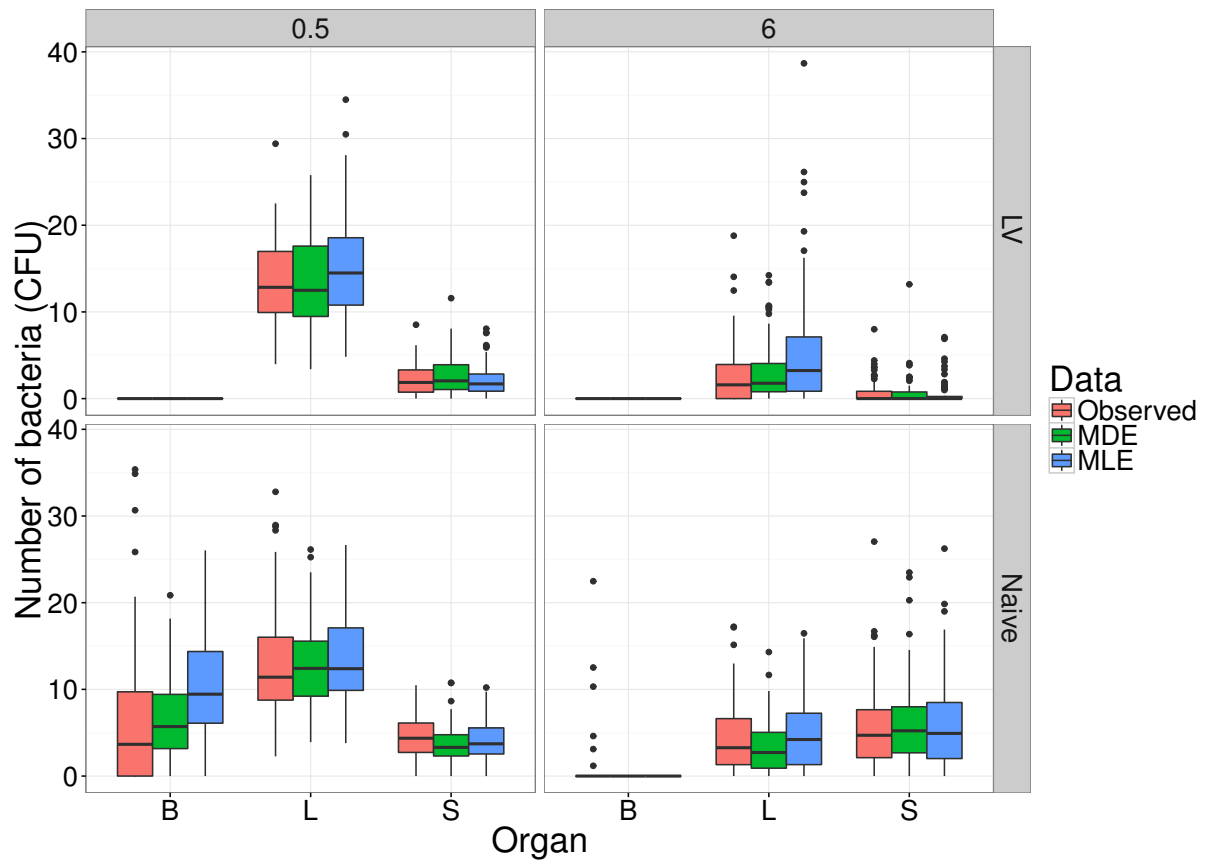
negligible discrepancy between the model output for the naive group fit, and the observed data. This suggests that some of the assumptions in the original dynamic model may be erroneous; however, revisiting them goes beyond the scope of the present study.

As a further demonstration of the model goodness-of-fit, we compare the model output at each of the estimated parameter sets, to the observed data. Figure 13 shows these simulations from each of the MDE and MLE approaches, at each of the 0.5h and 6h observation times, for both the naive and vaccinated experimental groups. Observational noise consistent with that in the experimental data was added to the simulated data (i.e., binomial sampling for observed counts, and log-normal noise consistent with qPCR). The plots indicate that the main source of discrepancy between data and model in the naive-mice group is the distribution of bacterial loads in the blood after 6 hours.

## 4 Discussion

We have described a functional and flexible moments-based method to estimate parameters of stochastic metapopulation models, and applied it to experimental data on within-host bacterial infection dynamics. Compared to simulation-based methods, our technique delivers accurate estimation orders of magnitude faster. Although simulation-based inference has grown in popularity in computational biology—either within likelihood-free [17] or approximate-likelihood [16] approaches— even with the increasing availability of fast, multi-core computers, algorithms can still take days to converge in multi-parameter and multi-variable problems. While this is not a major issue when fitting a single model to a single dataset, it is a hindrance for more ambitious applications: indeed there is a growing demand in biology for model selection and model-based optimal experimental design, which are much more computationally intensive tasks (e.g., [34, 35, 36, 37]).

In its current form, our method can incorporate any linear, multivariate, continuous-time Markovian model, and fit it to experimental data that include multiple replicates and an arbitrary number of independent time points. These last two characteristics are typical of experimental biology, yet little attention has been given to systems of this form in recent statistical developments. Indeed, many inference methods for stochastic models



**Figure 13:** Observed experimental data for both naive and vaccinated groups, at both observation times, compared to simulations from the model at parameters estimated by both the MLE and MDE methods, in each of the blood (B), liver (L) and spleen (S). Numbers of bacteria are the sums of eight identical WITS.



489 (for example, driven by applications to epidemiology), target inference from a single time-  
490 series [38, 16].

491 In addition, we have provided a worked example for how to correct for observation  
492 noise, applicable to any given experimental system. While sampling error is typically  
493 taken into account in likelihood-based inference, many inference studies either ignore  
494 experimental noise (e.g. [24]) or choose arbitrary distributions (e.g. [39]). Even if ex-  
495 perimental error has limited impact on the mean of the observations, it will affect the  
496 variance, with implications for the precision and reliability of statistical inference. The  
497 method we demonstrated here is based on pre-processing experimental data to effect an  
498 empirical correction of the observation noise. Crucially, it is not limited by mathematical  
499 tractability when combining multiple error sources, and it does not slow down the infer-  
500 ence computation (i.e., it only needs to be performed once before fitting the model, and  
501 the same simulations are also used to adjust the moments of the noisy-simulated data).

502 The choice of a metric to minimise for likelihood-free inference is a common issue  
503 in computational statistics, especially in the context of increasingly popular ABC meth-  
504 ods [40]. When the data and the model output are summarised by multiple statistics,  
505 the default option is to use either euclidian distance or a chi-squared type variant. The  
506 latter was chosen, for example, in a recent study using moment-based inference to solve a  
507 systems-biology problem [24]. However, because the summary statistics of interest are the  
508 moments of statistical distributions, we hypothesised it would be more informative to use a  
509 divergence metric instead. While many divergence measures exist for the purpose of com-  
510 paring mathematically defined distributions [41], we are not aware of standard methods to  
511 compute divergence between multivariate distributions generated by complex stochastic  
512 processes. Instead, we took a pragmatic approach and used mathematical expressions  
513 for the Hellinger distance or the Kullback-Liebler divergence between multivariate normal  
514 distributions, because these expressions depend on the first- and second-order moments of  
515 the distributions only. Even though the resulting divergence measures are not the actual  
516 Hellinger distance or Kullback-Liebler divergence between our observed and predicted  
517 distributions, they still outperform the chi-squared metric based on parameter inference  
518 accuracy. It is worth noting that, across the three model structures we tested, there

519 was not a single metric that was consistently better than any other, and the differences  
520 in accuracy were often relatively small (Fig. 5). Depending on the degree of accuracy  
521 sought, it may be worth testing these and other metrics against simulations before apply-  
522 ing this method to a different experimental system. It is our intention to provide a flexible  
523 blueprint that can be tailored to other problems, rather than a one-size-fits-all black box  
524 which may prove unreliable as soon as the circumstances change.

525 The particular molecular technology (isogenic tagging) that motivated the develop-  
526 ment of this inference method, has become pervasive in the study of within-host dynamics  
527 of bacterial infection in the last 10 years (see reviews by [42, 2, 43]). Yet, to our knowl-  
528 edge, this is the first attempt to provide a general modelling and inference framework  
529 that could be applied to any of these experimental systems. Indeed, previous efforts have  
530 been tailored to specific case studies [43, 7, 9, 13, 44, 8] despite asking fundamentally  
531 similar questions: how fast are bacteria replicating and dying? How much migration is  
532 taking place among organs or tissues? As soon as any two of these dynamic processes are  
533 co-occurring, it is not possible to evaluate them based solely on average bacterial loads: it  
534 is necessary to obtain reliable estimates of the variance, preferably within a single animal,  
535 by quantifying a set of independent and isogenic tags. The first known example goes back  
536 60 years, using two naturally occurring mutants of *S. enterica* that could be distinguished  
537 by selective growth medium to investigate colonisation dynamics in mice. Although a  
538 wide range of bacterial tagging methods (including antibiotic markers and fluorophores)  
539 have been used since, non-coding DNA barcodes have opened new prospects as arbitrarily  
540 large numbers of truly isogenic tags can be generated and quantified by sequencing [14].  
541 It is our hope that the inference framework presented here will contribute to the field's ex-  
542 tension by providing much needed analytical support to analyse and design microbiology  
543 experiments.

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547 Maskell. We are also grateful to fellow modellers Roland Regoes, Simon Frost, Julia Gog  
548 and Joshua Ross for their technical advice.

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