Energy Exchanges at Contact Events Guide Sensorimotor Integration 1 2 **Across Intermodal Delays** Ali Farshchiansadegh^{1,2,*}, Alessandra Sciutti ^{2,3}, Assaf Pressman ⁴, Ilana Nisky ^{4,5}, and 3 Ferdinando A. Mussa-Ivaldi ^{1,2,6,7} 4 5 ¹Department of Biomedical Engineering, Northwestern University, Evanston, Illinois, USA 6 ²Sensory Motor Performance Program, Rehabilitation Institute of Chicago, Chicago, Illinois, USA 7 ³Department of Robotics, Brain and Cognitive Sciences, Italian Institute of Technology, Genoa, Italy 8 ⁴Department of Biomedical Engineering, Ben-Gurion University of the Negev, Be'er Sheva, Israel 9 ⁵Zlotowski Center for Neuroscience, Ben-Gurion University of the Negev, Be'er Sheva, Israel 10 ⁶Department of Physical Medicine & Rehabilitation, Northwestern University, Chicago, Illinois, USA 11 ⁷Department of Physiology, Northwestern University, Chicago, Illinois, USA *Correspondence: a-farshchiansadegh@northwestern.edu 12

ABSTRACT

One must know the mass of an object to accurately predict how it moves under the effect of an applied force. Similarly, the brain must represent the arm's inertia to predict the arm's movements elicited by commands impressed upon the muscles. Here, we present evidence suggesting that the integration of sensory information leading to the representation of the arm's inertia does not take place continuously in time but only at discrete transient events, in which kinetic energy is exchanged between the arm and the environment. We used a visuomotor delay to induce cross-modal variations in state feedback and uncovered that the difference between visual and proprioceptive velocity estimations at isolated collision events was compensated by a change in the representation of arm inertia. The compensation maintained an invariant estimate across modalities of the expected energy exchange with the environment. This invariance captures different types of dysmetria observed across individuals following prolonged exposure to a fixed intermodal temporal perturbation and provides a new interpretation for cerebellar ataxia.

INTRODUCTION

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In a conference if you cannot understand the speaker due to excessive background noise or poor acoustics, seeing her face would help you capture what she is saying. The evident explanation for this experience is that the integration of information from multiple sensory modalities improves perception (Ernst and Bülthoff 2004). Similarly, the sensorimotor control system combines different sensory measurements to enhance the perception required to perform accurate movements and to skillfully manipulate objects. However, because of delays in neural pathways, the brain cannot rely entirely on sensory feedback to effectively control movements, particularly when interacting with a dynamical environment. Predicting the consequences of an action is essential to compensate for the temporal delays of sensory information. To this end the brain relies on internal representations, or "internal models" of the body and of the environment in which it operates (Wolpert, Ghahramani et al. 1995, Miall and Wolpert 1996, Wolpert and Kawato 1998, Kawato 1999). The predictions of these internal models, often called forward models, generate expectations for future sensory consequences of the ongoing motor commands before sensory feedback becomes available (Shadmehr, Smith et al. 2010). These "priors" are combined with delayed sensory feedback to estimate both the state (e.g. position and velocity) of the body and the context (e.g. mass of manipulated object) of the movement (Wolpert and Ghahramani 2000, Wolpert and Flanagan 2001). In a biological system, however, noise and uncertainty spread through every aspect of sensory perception and motor command generation (Faisal, Selen et al. 2008). Additionally, the environment itself is ambiguous and variable. This makes state and context estimation probabilistic problems to solve. Over the past decade, Bayesian integration theory has provided a unifying framework to capture behavior under uncertainty in a wide range of psychophysical studies on sensory perception (Weiss, Simoncelli et al. 2002, Jazayeri and

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Shadlen 2010), multisensory integration (Ernst and Banks 2002, Alais and Burr 2004, Ernst 2007), and sensorimotor function (Körding and Wolpert 2004, Miyazaki, Nozaki et al. 2005). However, the temporal structure of state and context estimation remains largely unknown. Object manipulation is an effective and natural test bed for sensorimotor integration. It engages multiple sensory modalities and in contrast to movements in free space, it provides an additional challenge to the nervous system. Holding an object changes the dynamics of the arm, thereby successful manipulation requires not only knowledge of the arm dynamics, but also knowledge of the object dynamics. This knowledge is not solely acquired through proprioceptive and tactile feedback; vision also provides information about the mechanical properties of the object (Gilden and Proffitt 1989, Gordon, Forssberg et al. 1991, Jenmalm and Johansson 1997, Salimi, Frazier et al. 2003, Ingram, Howard et al. 2010, Takamuku and Gomi 2015). Here we employed an object manipulation task to investigate the temporal resolution of the sensory integration process that provides the information for estimating the mechanical properties of the object being manipulated (i.e. context estimation). We considered two possibilities: a time-dependent structure in which context estimation takes place continuously or periodically at isochronous intervals and a statedependent structure in which context estimation occurs sporadically at salient task-relevant events (e.g. contact events in an object manipulation task). To test these alternative possibilities, we developed a virtual two-dimensional ping-pong game in which participants continuously manipulated an object (paddle) to hit a ball (**Figure 1A**). Visual, haptic, and auditory feedbacks were provided simultaneously at the time of impact between the paddle and the ball. This design was ideal for our purpose as it was a continuous object manipulation task that also included discrete multisensory events. In this task, the two proposed temporal structures would provide different mass estimations after adaptation to an artificial delay

in the sensory feedback (Foulkes and Miall 2000, Miall and Jackson 2006, Farshchiansadegh, Ranganathan et al. 2015). **Figure 1B** is a schematic illustration of the changes in the hand position during stroke and recovery in the pong game with its delayed visual representation. If proprioceptive and visual information are integrated continuously or periodically to estimate the mass of the paddle, then the internal representation of the mass should remain unchanged at the end of adaptation. This is because the mismatch between the two sensory measurements would integrate to zero (integrating over the region indicated by the gray box in **Figure 1B**) not only for position, but also for all the higher derivatives. On the other hand, if sensory integration for mass estimation occurs only at collision events, then this should result in predictable and systematic changes in the mass representation depending on the difference between sensory measurements at the time of events. To assess the changes in representation of mass, we asked participants to perform reaching movements without feedback (in a feedforward fashion) before and after playing pong.

RESULTS

We asked three groups of volunteers to make blind reaching movements to visual targets before and after playing a simulated pong game holding a robotic manipulandum. After playing pong for a few minutes without a delay, the game's response to the player's movements was delayed and participants continued playing for ~40 minutes. We investigated the effects of adaptation on the reaching trajectories.

Experiment I

The first group of participants played a frontal pong (FP, proximal-distal direction, **Figure 1A**). With practice, all subjects improved their performance. Since subjects were instructed to maximize the number of collisions with the ball, hit rate was set as a metric for proficiency. A paired t-test between the first and the last five minutes of the delayed pong, reveled a significant increase in the number of hits per minute (p = 0.04). Notably, playing the delayed pong influenced the reaching behavior. **Figure 1C** compares the endpoint of the reaches of a participant in this group before and after adaptation. A systematic hypermetria in reaching was observed in all subjects after playing the game (**Figure 1D**). The magnitude of the movements was significantly larger following adaptation (paired t-test, p = 0.02). To further verify that the changes in reaching trajectories are not a byproduct of interacting with the robot itself, a subgroup of the subjects in this group also participated in a control experiment in which the game was not delayed. Expectedly, the hypermetria was absent in this experiment (paired t-test, p = 0.60).

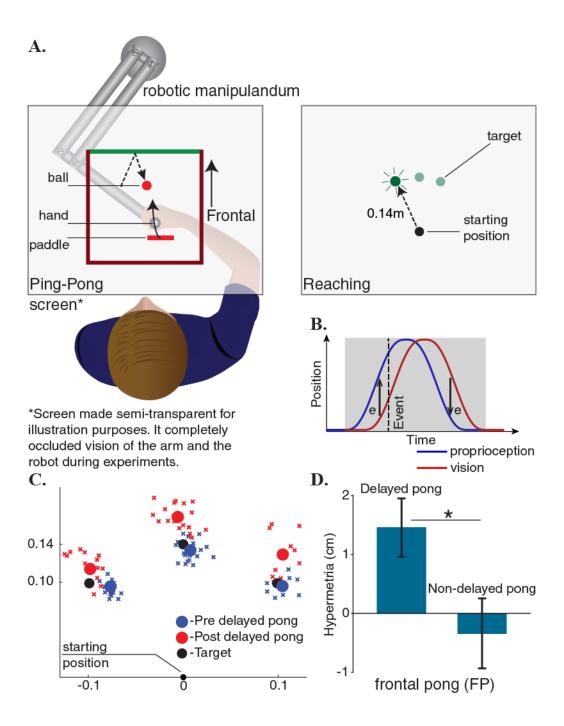


Figure 1. Adaptation to delayed feedback in a ping-pong game influences reaching behavior. (**A**) Subjects played a planar pong game in frontal direction using a robotic manipulandum. In addition to continuous visual feedback, auditory and tactile feedbacks were provided simultaneously upon collisions with the ball. After few minutes of familiarization, the game's response to the player's movements was delayed and subjects continued playing the game in the delayed environment. Participants also performed reaching movements without any continuous or terminal feedback before and after playing the pong. Objects and labels in black were not visible to the subjects (**B**) A cartoon of the changes in the hand position during stroke and recovery in the pong game and its delayed representation. If sensory integration occurs continuously, then the reaching trajectories should remain unchanged after adaptation. Because the difference between visual and proprioceptive information integrates to zero. However, if sensory

integration occurs only at collisions, this should result in predictable changes in the terminal position of the

reaching movements depending on the sensory measurements at collisions. (C) The endpoints of the reaching movements of a typical subject before and after adaptation. (D) All subjects showed hypermetria in the reaching movements after adaption. The hypermetria was absent in a subgroup who additionally did the same experiment without the delay. Error bars represent one standard error of the mean.

One interpretation of these results would suggest that adapting to the delay changed the representation of the mass of the object (paddle) being manipulated. In this case, hypermetria would follow from assigning inertial values to the object that are higher than the actual value. However, there were multiple alternative interpretations including different kinematic models (see the discussion section) that were similarly successful to explain this outcome. To consider these alternative explanations, we designed a lateral pong game. The main objective of the lateral pong was to create a scenario in which two groups play the game under similar kinematic conditions but with paddles that possess different mechanical properties. To this end, we took advantage of the passive dynamics of the robot.

Experiments II & III

In these experiments, we placed two pong courts next to each other and participants played a lateral pong (LP, medio-lateral direction, **Figure 2A**). One group played the delayed pong only in the right court (LP_R), while the other group played the delayed pong only in the left court (LP_L). The same pattern of reach targets that was utilized in the experiment I were re-positioned within each court (**Figure 2A**). Both groups performed blind reaching movements to all six targets from the corresponding starting positions in each court before and after adaptation. To ensure that the difficulty level of playing pong was not different between the courts, initially all participants played the game with no delay in both courts. Hit rate analysis showed that there was no difference in performance across the courts (paired t-test, p = 0.32). Thus, we could assume that there was not an inherent gap in difficulty between the two courts. Task performance was drastically affected

when the delay was introduced. However, with practice both groups improved their performance significantly at an equivalent level. A mixed-design ANOVA with practice as a within-subject factor (2 levels) and group as a between-subject factor (2 levels) revealed a main effect of practice (F(1,14) = 55, p < 0.001), no effect of group (F(1,14) = 0.007, p = 0.93) and no interaction effect (F(1,14) = 2.1, p = 0.17).

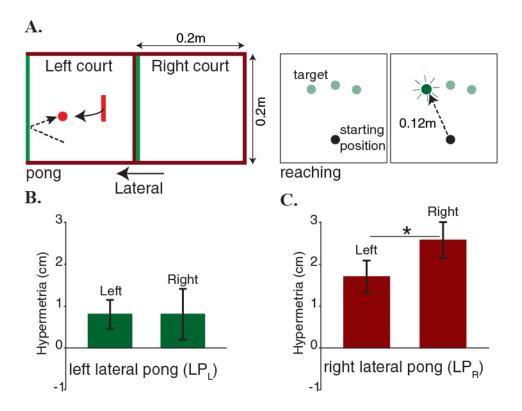


Figure 2. Hypermetria in reaching depends on the dynamics of the pong. (**A**) Two separate groups of subjects played a lateral pong with delay. Each group adapted to the delay only in one of the two courts that were placed next to each other. Both groups performed blind reaching movements before and after adaption from starting positions on the two sides of the body midline. Objects and labels in black were not visible to the subjects. (**B**) Subjects on the left court showed a very small average hypermetria on both sides. (**C**) Subjects on the right court showed a large average hypermetria on the right side that generalized to a lesser extent to the left side. Error bars represent one standard error of the mean.

While the learning rates and the level of performance were largely equivalent across the two groups, the effect of adaptation on the reaching trajectories was strikingly different: the LP_R group demonstrated a large hypermetria on the right side (the training region) that generalized to a lesser

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extent to the other side (**Figure 2C**), whereas the LP_L group showed only a very small hypermetria on both sides (Figure 2B). A two-way mixed ANOVA on change in the movement magnitude, with reaching side as a within-subject factor (2 levels) and group as a between-subject factor (2 levels) revealed no significant main effect of reaching side (F(1,14) = 2.1, p = 0.17). However, there was a significant main effect of group (F(1,14) = 5.4, p = 0.035). Additionally, there was no significant interaction effect (F(1,14) = 2.1, p = 0.17). Further within group analyses indicated that there was a significant reduction of the overshoot as the LP_R group performed reaching movements on the left side and away from the training region (paired t-test, p = 0.04). This pattern was not present in the LP_L group because this group demonstrated a very small hypermetria on both sides that was not even significant on the training side (paired t-test, p=1). Sensory integration at events explains individual differences We have recently shown that when transporting an object carried by the hand, visual and proprioceptive information are integrated to optimize the kinetic energy transferred to the object (Farshchiansadegh, Melendez-Calderon et al. 2016). For the same optimization to occur in a pong game, it is necessary for the collisions to happen at the time of peak paddle velocity. Analysis on the relationship between the velocity profile and the collision time in the baseline non-delayed trials - when vision and proprioception were congruent - reveals that, here as well, participants adopted the energy-efficient strategy by hitting the ball, on average, at the time of peak velocity (Figure 3A). In adaptation trials, haptic (force impulse) and auditory feedback were also delayed. Therefore, as in the non-delayed game, each hit in the delayed game generated a simultaneous multisensory response. However, participants effectively played the game with two paddles that were separated in time: a visual paddle (delayed) and a proprioceptive paddle (not delayed). **Figure 3B** illustrates

the schematic velocity profile of the visual and the proprioceptive paddles for a movement in the hitting direction. For a hit that is happening at time t_1 in this figure, the kinetic energy at collision is related to the velocity of the proprioceptive and visual paddles as

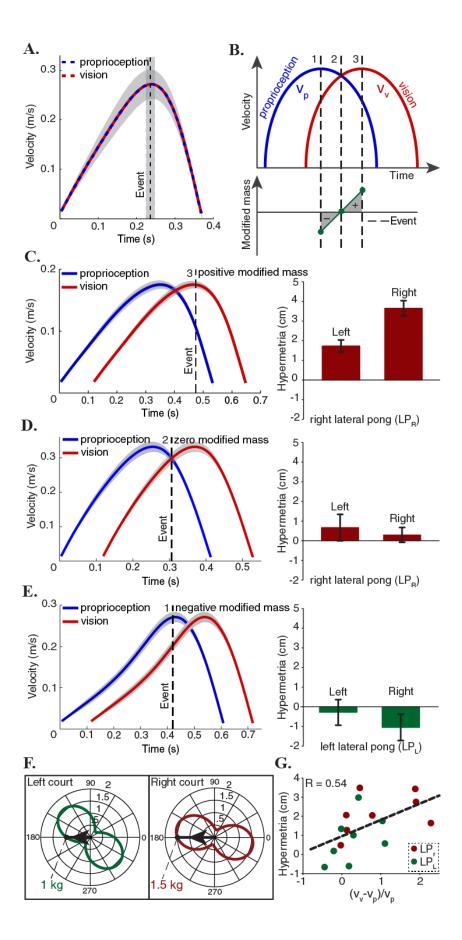
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$$KE(t_1) = \frac{1}{2}m_r v_p(t_1)^2 = \frac{1}{2}m_r v_p(t_1 - \tau)^2 \neq \frac{1}{2}m_r v_p(t_1)^2$$
 (1)

Where m_r , v_v , v_p and τ represent the effective mass of the robot, the velocity of the visual paddle, the velocity of the proprioceptive paddle and the delay, respectively. Also, note that at time t_1 the estimate of the kinetic energy of the paddle based on visual information would be different from the estimate based on proprioceptive information because the velocity measurements are different in the two modalities. We hypothesize that sensory integration for mass estimation does not happen continuously in time but only at salient multisensory events when there is an exchange of kinetic energy with the environment, in this case at collisions. Moreover, we hypothesize that the optimization problem must satisfy the constraint that the estimated kinetic energy transfer remains invariant across modalities. Therefore, instead of estimating τ one may rewrite equation (1) without explicit consideration of the delay, by modifying the effective proprioceptive mass of the robot (see the methods section for the definition of effective mass and its connection to kinetic energy):

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$$KE(t_1) = \frac{1}{2}m_r v_v(t_1)^2 = \frac{1}{2}(m_r + \widehat{m}) v_p(t_1)^2$$
 (2)

Under this hypothesis, discrete sensory integration at isolated collision events leads to a perceptual illusory mass \hat{m} , that hereinafter we refer to as "modified mass" and can be derived from equation (2) at any hitting time:

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$$\widehat{m} = m_r \frac{v_v(t_{hit})^2 - v_p(t_{hit})^2}{v_p(t_{hit})^2}$$
 (3)



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Figure 3. Modified mass explains individual and group differences. (A) Subjects optimized the energetic cost of their movements in the non-delayed pong game by hitting the ball at the peak velocity of the paddle. (B) In the delayed pong, visual and proprioceptive measurements were different at the time of collisions. Hence, sensory integration at events caused a misperception of the paddle's mass. Modified mass is the difference between the actual mass and the perceived mass. Depending on the timing of the hits, modified mass can have three categorical values: a hit around time 1 leads to a negative modified mass $(v_v < v_p)$, a hit at time 2 $(v_v = v_p)$ makes the modified mass to be zero and for a hit around time 3 $(v_v > v_p)$, the modified mass is positive. (C-E) Left panels show the average velocity profile of the hand and the paddle during the last five minutes of adaptation for three individual subjects, one from each possible outcome category. The vertical dashed line represents the average time of the hit in the pong game. Right panels show the adaptation effects on the reaching movements. Error bars represent one standard deviation of the mean. These results are consistent with the hypothesis that mass estimation occurs at discrete events. (F) Effective mass of the manipulandum in each direction. Each plot is centered on the average position of the hits for the corresponding group. Subjects in the LP_R group played with a heavier paddle than the LP_L group. In addition, the modified mass is proportional to the mass of the paddle itself. Collectively, these two facts explain the group differences in the lateral pong experiments. (G) Correlation between the extent of hypermetria in the reaching movement and the average hitting time during the pong for all subjects. Gray areas represent 95% confidence intervals. Depending on the time of collision, the modified mass can have three categorical values (Figure **3B**): a hit that happens around time 1 leads to a negative modified mass since around this time $v_v < v_p$, a hit at time 2 ($v_v = v_p$) makes the modified mass to be zero and finally if the hit happens around time 3 ($v_v > v_p$), the modified mass would be positive. Previously, we examined the changes in the reaching movements following adaptation at the group level. As it is typically the case, there was a substantial variability in the performance of each participant following adaptation. The hypothesis that estimation of the effective mass depends on the sensory measurements at contacts allows us to make predictions of individual responses. To test this prediction, we consider within each group cases that deviated maximally from the average behavior. Figure 3C corresponds to the subject that exhibited the largest hypermetria in the LP_R group (right panel). Our hypothesis predicts that the timing of the collisions for this individual should be around time 3 because the large hypermetria indicates a positive estimation of the modified mass and thereby an increase in the perception of the robot's effective mass. Analysis

on the pong data confirmed this prediction: the left panel of this figure shows the average velocity profile of the two paddles during the last five minutes of adaptation for this subject and the vertical dashed line represents the average time of the hit. On the other extreme of the LP_R group, the individual in **Figure 3D** did not show an effect. Similar analysis on the pong data showed that on average this subject hit the ball at time 2 where the two velocities were equal. Per our hypothesis this would cause the modified mass to be zero. The subject that exhibited the largest hypermetria in the LP_L group behaved similarly as their counterpart in the LP_R group by timing the strokes in a same manner to hit the ball at around time 3 (same as **Figure 3C**). Finally, the other extreme subject in the LP_L group showed a notable hypometria on the right side (**Figure 3E**). In this case, the hypothesis predicts a negative estimation of the modified mass which is a consequence of the impacts that are occurring at around time 1. Subsequent analysis of the velocity profiles and the average hitting time of this subject corroborated with this prediction as well. Figure 3G is a scatter plot of all subjects that shows the dependence of their hypermetria on the average hitting time. Indeed, there was a significant correlation between the timings of the hit in the pong game and extents of overshoot in the reaching task among all participants (F = 5.6, p = 0.03). Thus far, we showed that sensory integration at events explains individual differences in all the three possible categories.

Mass of the manipulated object explains group differences

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The lateral groups played the game in the same direction with the same amount of delay and there were no differences in performance and adaptation rate between the two groups. However, despite the equivalence of the task in the right and left courts, the effect of adaption on the reaching trajectories was asymmetric between these two groups at the end of the experiment. This asymmetry is explained by the change in the dynamics of the task. The effective endpoint mass of

the five-bar linkage robotic device used in this study depends on the configuration and the direction of motion. These dependencies can be portrayed by polar plots that are centered at any desired configuration. Each point on the plot represents the projection of the inertia matrix onto the direction (unit velocity vector) that connects the center to that point. **Figure 3F** illustrates two of these plots that are centered on the average position of the hits with arrows that indicate the average movement direction across all subjects in each lateral pong group. This analysis reveals that the subjects in the LP_R group played with an apparently heavier paddle with the effective mass of a 1.5kg, compared to the LP_L group, whose paddle had the average effective mass of a 1kg. We know from (3) that the modified mass is directly proportional to the mass of the object being manipulated and therefore the larger hypermetria in the LP_R group can be explained by the fact that this group played with a paddle that had a larger effective mass than the LP_L group.

Model predictions

In the previous subsections, we laid out the elements that explain different outcomes at an individual and group level. Here, we present and validate a computational model that employs these concepts to predict the reaching behavior (see the methods section for a detailed description of the model). For each individual, we extracted the configuration of the robot, velocity of the visual paddle, and velocity of the proprioceptive paddle (hand's velocity) at impacts from the pong data. From these data, we computed the visual effective mass and the proprioceptive effective mass at hits and combined them by using maximum-likelihood estimation to obtain the modified mass. Next, we predicted the outcome of blind reaching movements after pong. To this end, we added the modified mass to the simulated model of the robot and computed the inverse dynamics for preplanned paths to the targets. We then used the calculated torques as feedforward commands to the actual model of the robot (without the modified mass) to replicate the blind reaching scenario.

Figure 4 illustrates the hypermetria in the simulated trajectories averaged across all subject in all the three groups. These predictions demonstrate the ability of this very simple computational model with only one free parameter (the modified mass) to capture the variance in the data: it explains between subject differences, the differences in the magnitudes of the hypermetria across groups and the reduction of the overshoot in the LP_R group on the left side.

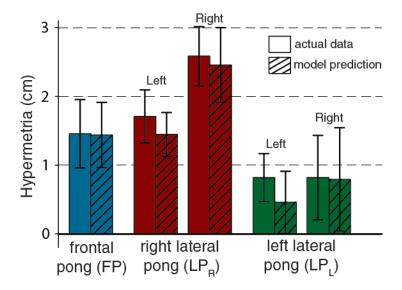


Figure 4. Model predictions. Predicted outcomes for all subjects in all three experimental groups.

DISCUSSION

We examined the temporal structure of the estimation process that is involved in the representation of object dynamics. Participants played a virtual pong game under an artificially induced visuomotor delay and performed reaching movements (without visual feedback) before and after the game using a robotic manipulandum. We predicted that a continuous or periodic estimation should result in no change in the internal representation of the robot's inertia whereas discrete estimation at contact events should lead to changes in the represented inertia. We found changes in the reaching trajectories after the game suggesting that participants estimated the mass only during contact events, at which kinetic energy was exchanged with the environment. These modifications in mass estimations appeared to conserve the expected exchange of kinetic energy across sensing modalities.

Alternative Explanations

However, there were other potential accounts for some of our observations. Introducing artificial delays between an applied force and the resulting motion causes an increase in the apparent mass of an object, as it alters the action-consequence relationship (Honda, Hagura et al. 2013). Modeling works has suggested that in the sensorimotor control system, externally imposed visual delays in the causal link between force and motion may be approximated by equivalent mechanical systems (Takamuku and Gomi 2015) such as a mass-spring-damper system (Sarlegna, Baud-Bovy et al. 2010). Therefore, an alternative explanation is that here as well the effect is due to an excessive delay in the visual response. But an important observation in these and other delay adaptation studies is that the overestimation of the mass fades with adaptation (Botzer and Karniel 2013, Honda, Hagura et al. 2013) and sudden delays in the visual feedback are necessary for the perception of additional mass (Takamuku and Gomi 2015). On the contrary, here the effect is a

consequence of prolonged exposure and adaptation. Another possibility is to interpret the results by considering the spatial effect of the imposed delay. A successful ball strike requires the paddle to be at a desired position within a certain time window. To achieve this objective in a delayed visual space, the hand needs to travel a longer distance, in the same time, and in the same direction. Therefore, the spatial distortions brought about by a visual delay can be approximated using a visuomotor scaling factor (Pine, Krakauer et al. 1996, Krakauer, Pine et al. 2000). Although with a fixed delay, the spatial expansion of the proprioceptive space is not uniform and the scaling factor depends on movement speed, it is reasonable to assume that the participants learned the average of the scaling factors that they experienced (Scheidt, Dingwell et al. 2001, Braun, Aertsen et al. 2009). The results from the lateral pong experiments allowed us to rule out these alternative possibilities. Two groups of participants played the game with identical kinematics while holding simulated paddles with different inertial mass. After adaptation, they exhibited a significantly different pattern of reaching performance suggesting that the mass of the paddle is a factor affecting the results. This asymmetric outcome eliminates the class of kinematic models including the scaling model. The free parameters in the mechanical equivalent model are also derived using the kinematics (position, velocity, and acceleration) of the object and its delayed representation. Therefore, this model also predicts an equal additional mass to be perceived by the groups. Moreover, none of these models can account for individual differences among the participants. Finally, we showed that a simple event-based estimation model can account for all the features of the experimental data.

Multisensory Events in Object Manipulation

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Many discrete events in the physical world are perceived through multiple sensory modalities providing us with different types of information regarding those events. Although these sensory stimuli originate synchronously in the environment, to perceive them as simultaneous the nervous system should, and in fact does, account for the differences in both physical (Sugita and Suzuki 2003) and neural (Stone, Hunkin et al. 2001) transmission rates. Additionally, the neural mechanism of simultaneity perception is subjective (Vroomen and Keetels 2010) and the temporal intermodal alignment can be recalibrated (Fujisaki, Shimojo et al. 2004). This adaptive mechanism is proposed to be beneficial for object manipulation purposes (Johansson and Flanagan 2009). Manipulation tasks often include distinct action phases in which objects are grasped, moved, brought in contact with other objects and released. These action phases are confined between discrete contact events that generate multi-sensory responses which are linked in space and time (Flanagan, Bowman et al. 2006, Johansson and Flanagan 2009). Therefore, sensory integration at these events provides a more accurate and reliable perception of the environment. In this study, we have provided experimental evidence to suggest that the nervous system exploits this opportunity by limiting the context estimation to sensory information provided at multimodal events. When reaching to grasp objects, the brain predicts the sensory consequences of contacts and estimate the level of the required grip force before they happen (Flanagan and Beltzner 2000, Flanagan, Vetter et al. 2003) using the experience of the previously manipulated objects (Haruno, Wolpert et al. 2001). Contact events are rich sources of information to compare the predicted and actual sensory responses. Therefore, forward models can be updated and aligned using prediction errors and context estimation at events. Depending on the complexity of the interactions and past experiences, occasional regulation of the forward models at events could be sufficient to fulfill and

attain the manipulation objectives. Indeed, this was the observation in the current study. Research on eye-hand coordination in sequential object manipulation tasks reported that participants direct their gaze to successive contact locations that mark the end of a sequence well before the time that hand reaches them (Johansson, Westling et al. 2001, Flanagan and Johansson 2003). But the gaze location remains fixed and stationary until the sequence is completed. These results indicate that the sensorimotor control system is actively seeking for task-relevant events that provide distinct and simultaneous multi-sensory information to compare and regulate forward model predictions for the upcoming manipulation sequence, while being confident that the previous event-based adjustments were adequate to attain the objective of the current sequence without any additional use for feedback. This event-driven use of state feedback in sensorimotor control has obvious computational advantages over a control scheme that continuously incorporates feedback.

Generalization

We put forward that the event-driven employment of feedback for context estimation and forward models calibration is not limited to contacts. External perturbations and inaccurate forward models lead to performance and prediction errors that require correction. Feedback is then integrated only after an event indicates that the control error exceeded some threshold. This threshold is variable and depends on feedback uncertainty (Wei and Körding 2010), perturbation uncertainty (Izawa, Rane et al. 2008) and the level of precision that is required by the task itself. Therefore, similar to the contact events, error events adjust forward models only in task-relevant dimensions. This task dependent use of feedback allows forward models to drift in the task-irrelevant dimensions (uncontrolled manifold) over time (Scholz and Schöner 1999, Todorov and Jordan 2002). In novel object manipulation tasks, when there are no forward models to rely on, feedback is extensively

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utilized at initial stages to train forward models whereas practice reduces reliance on feedback (Sailer, Flanagan et al. 2005). We propose that the features that we discussed so far regarding context estimation can be generalized to state estimation. Ariff and colleagues (Ariff, Donchin et al. 2002) designed an experiment in which they asked participants to track with their eyes the location of their own unseen hand during reaching movements and they found a proactive gaze behavior with gaze leading the hand. In this task, forwards models and proprioceptive feedback were combined to estimate the state of the hand and eye movements were served as a proxy for the estimation process. An important observation in this study - for our purposes here - is that rather than pursuit eye movements, participants made saccades to track the hand (but see (Gauthier and Mussa Ivaldi 1988, Gauthier, Vercher et al. 1988)). Moreover, the position and timing of these saccades were random. Therefore, even in simple and familiar reaching movements, the task demands for continuous state estimation could not be satisfied. The role of cerebellum in event prediction and formation of forward models The adaptive learning mechanism in the cerebellum (Marr and Thach 1991) makes it an ideal substrate for generating forward models. There is growing body of evidence from studies on behavioral deficits in patients with cerebellar dysfunction (Bastian, Martin et al. 1996, Tseng, Diedrichsen et al. 2007), functional imaging (Blakemore, Frith et al. 2001, Kawato, Kuroda et al. 2003), and transcranial magnetic stimulation (Miall, Christensen et al. 2007, Schlerf, Galea et al. 2012) that links the cerebellum to forward models (Bastian 2006). In a ball catching task, subjects with cerebellar damage exhibited difficulty in predicting the required muscle forces to compensate for ball weight before the ball reached the hand, but showed normal force adjustments after impact (Lang and Bastian 1999). Similarly, in a locomotion study (Morton and Bastian 2006), Subjects

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with cerebellar damage were capable of making reactive changes to a perturbation, but were impaired at making predictive adjustments. In object manipulation, cerebellar lesions prevented predictive grip force modulations in anticipation of inertial loads (Nowak, Hermsdörfer et al. 2002, Rost, Nowak et al. 2005). These results suggest that the integrity of the cerebellum is critical for preparing motor responses in anticipation of discrete sensory events that mark the transition between action phases. Damages to the cerebellum impairs adaptation to both kinematic (Martin, Keating et al. 1996) and dynamic (Smith and Shadmehr 2005) changes in the environment. Persons with cerebellar ataxia may exhibit dysmetria in their movements. The dysmetria have a distinctive character in each individual. Some tend to show hypometria, while others are hypermetric (Manto 2009). It has recently been shown that errors in movement extent in patients with cerebellar dysmetria is caused by the misrepresentation of arm dynamics (Bhanpuri, Okamura et al. 2014). Our findings here suggest that errors in estimating mechanical properties of the arm could be caused by the cerebellar dysfunction in temporal processing and alignment of multimodal sensory information. Moreover, each injury to the cerebellum, depending on the location and severity, leads to a specific temporal calibration error in sensory integration causing a broad range of patient specific motor deficits.

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METHODS Participants Twenty-four right handed volunteers (11 females, ranging in age from 23 to 35) participated in the study. All participants were neurologically intact with normal or corrected to normal vision and had no prior knowledge of the experimental procedure. The study protocol was approved by Northwestern University's Institutional Review Board and all the participants signed an informed consent form. Experimental setup Participants were positioned in front of a horizontal screen and held the handle of a planar, two degree of freedom robotic manipulandum with their right hand. The screen prevented the participant's view of their arm and the robot. A projector was used to display the visual information on the screen and it was calibrated so that the position of the handle was overlaid on its true position with a precision of 1 mm. Position and velocity of the robot were computed from instrumented encoders at the frequency of 1 kHz to provide sensory feedback during the experiment and the data were recorded at the rate of 200 Hz. Experimental design The experiment consisted of two tasks: playing a pong game and executing reaching movements. In the pong game, the ball movement was confined to a rectangular court and participants were instructed to hit the ball towards a side that was distinguished by a different color (green sides in Figure 1A and Figure 2A) from the remaining sides using a rectangular paddle that represented the location of the hand. To expand the court coverage and to mimic the presence of an opponent, the velocity of the ball was changed by a random number upon bouncing from the distinguished side of the court. This number was drawn from a uniform distribution between ± 0.13 m/s and was applied to the velocity component along the bouncing side. Additionally, friction was modeled as a linear decay in the velocity of the ball. After a collision with the paddle, the ball velocity was determined using

$$\begin{bmatrix} \dot{x}_{ball}^{+} \\ \dot{y}_{ball}^{+} \end{bmatrix} = 0.7 \begin{bmatrix} \cos 2\theta & \sin 2\theta \\ \sin 2\theta & -\cos 2\theta \end{bmatrix} \begin{bmatrix} \dot{x}_{ball}^{-} \\ \dot{y}_{ball}^{-} \end{bmatrix} + 0.42 \begin{bmatrix} \dot{x}_{paddle} \\ \dot{y}_{paddle} \end{bmatrix}$$
(4)

Where – and + represent before and after the collision respectively and θ is the orientation of the paddle with respect to the horizontal axis. A haptic pulse was generated by the robot at the time of impact for the duration of 5 ms. This force feedback was computed using $f = 0.01\Delta v_{ball}$, where Δv is the change in the velocity vector. The sudden activation of the motors to generate this pulse was creating a sound that made it unnecessary to provide any additional auditory feedback. Each trial of the pong game lasted for one minute. A timer indicated the elapsed time and a counter displayed the number of collisions in each trial.

In the reaching phase, the screen turned black and a circular target appeared on the screen. Participants were instructed to reach the target and stop there. This movement was executed without a visual feedback of the location of the hand and it was guided only by the proprioceptive representation of the hand position in relation to the visual target. After the movement was complete, the hand was passively brought back to the starting position by the robot. Similarly, no visual feedback of the starting position was present.

Protocol

Participants were divided in three groups. All the experiments consisted of a reaching-pongreaching sequence. Participants in the first experiment (n = 8), played pong in frontal direction (**Figure 1A**). After two minutes, the game was delayed for $\tau = 80$ ms and participants played the delayed game for ~40 minutes. The delay was applied across all the visual, haptic, and auditory

channels. In reaching tasks, participants performed 45 reaching movement in a random order to three targets that were placed at 0.14 m from the starting position and were separated from each other by 45° (**Figure 1A**). A subgroup of participants in this experiment (n = 5), also participated in a control experiment in a separate session where they played the game for ~20 minutes but without the pong being delayed. The order in which these participants performed the delayed and non-delayed game was randomized. In the two other experiments, participants played pong in lateral direction. Two pong courts where juxtaposed next to each other (Figure 2A) in such a way that their intersection was along the participants' body midline. At the beginning, participants played the pong game with no delay in both courts for the total time of eight minutes that was equally divided and alternating between the courts. Next, participants in one group (n = 8) played the delayed pong only in the right court for 40 minutes, while the other group (n = 8) played the delayed pong only in the left court for the same amount of time and with the same amount of delay ($\tau = 120 \text{ ms}$). However, the reaching tasks before and after pong were identical across these two groups, we duplicated the same pattern of targets that was used in the first experiment and placed one in each court (Figure 2A). Therefore, participants in these two groups performed reaching movements to six targets (three in each court) from two corresponding starting positions (one in each court). Each movement was

Computational model

repeated 5 times in a random order.

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The equations of motion for a five-bar linkage robotic device used in this experiment can be derived using the Euler-Lagrange equations and expressed in matrix form as

$$M(q)\ddot{q} + C(q, \dot{q})\dot{q} = u \tag{5}$$

Where M(q), $C(q,\dot{q})$ and u represent the inertia matrix, Centripetal/Coriolis matrix and generalized forces respectively. The effective mass of the robot is spatially varying and configuration dependent. The effective mass (m_r) is defined as the projection of the inertia matrix onto the instantaneous direction of motion (Worsnopp, Peshkin et al. 2006). Therefore, for each direction of motion at each configuration, the inertia of the robot matches that of a point mass. The inertia of this equivalent point mass can be derived using the conservation of energy principle: the kinetic energy of the robot must be equivalent to the kinetic energy of the point mass

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$$\frac{1}{2}\dot{\boldsymbol{q}}^{T}\boldsymbol{M}(\boldsymbol{q})\dot{\boldsymbol{q}} = \frac{1}{2}\dot{\boldsymbol{x}}^{T}m_{r}\dot{\boldsymbol{x}}$$
 (6)

The unit velocity vector is $\dot{x} = [\cos \theta \sin \theta]^T$ and θ is the angle between the direction of motion and the x-axis. Therefore

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$$m_r = \dot{x}^T (J^{-1}(q))^T M(q) J^{-1}(q) \dot{x}$$
 (7)

Where J is the Jacobian matrix. To predict the outcome of blind reaching movements after pong we extracted the configuration of the robot, the velocity of hand (v_p) and its delayed representation (v_v) at hits from the pong data during the last five minutes of adaption for each individual. From these data, we computed the effective visual mass $(m_v = m_r)$ and the effective proprioceptive mass $(m_p = m_r \frac{v_v^2}{v_p^2})$ of the robot. Next, we integrated these sensory information using maximum-likelihood estimation (Ernst and Banks 2002) to obtain the apparent mass

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$$E(m) = \frac{1/\sigma_v^2}{1/\sigma_v^2 + 1/\sigma_v^2} m_v + \frac{1/\sigma_p^2}{1/\sigma_v^2 + 1/\sigma_v^2} m_p$$
 (8)

Where σ_v^2 and σ_p^2 represent the variance of the effective visual and proprioceptive masses at hits.

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The perceived mass is therefore different from the actual effective mass of the robot. We called this difference the modified mass $(\widehat{m} = E(m) - m_r)$. Finally, we added the modified mass to the simulated model of the robot and computed the inverse dynamics for preplanned minimum jerk (Flash and Hogan 1985) trajectories to the targets. We then used the calculated torques as feedforward commands to the actual model of the robot (without the modified mass). The difference in the dynamic model of the robot between inverse computation and feedforward simulation caused an erroneous trajectory. The magnitude of the error was used to emulate changes in reaching trajectories after adaptation. Data and Statistical Analysis A fifth-order Butterworth low-pass filter with a cutoff frequency of 20 Hz was implemented to smooth the velocity signals. We fed the hit data from the last five minutes of pong to the computational model, however the output of the model was not sensitive to this choice. The hits at which the proprioceptive effective mass was more than ten standard deviations away from the mean visual effective mass were removed from the analysis. The threshold of significance in all the statistical analysis was set at 0.05.

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