Band Ratios

Title

Bectrophysiological Frequency Band Ratio Measures Conflate Periodic and Aperiodic Neural
 Activity

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6 Authors

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- 19 Donoghue & Voytek initiated and designed the study. Dominguez & Donoghue performed the
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- 37 possible.
- 38

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39 Abstract

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41 A common analysis measure for neuro-electrophysiological recordings is to compute the 42 power ratio between two frequency bands. Applications of band ratio measures include 43 investigations of cognitive processes as well as biomarkers for conditions such as attention-deficit 44 hyperactivity disorder. Band ratio measures are typically interpreted as reflecting quantitative 45 measures of periodic, or oscillatory, activity, which implicitly assumes that a ratio is measuring the 46 relative powers of two distinct periodic components that are well captured by predefined frequency 47 ranges. However, electrophysiological signals contain periodic components and a 1/f-like aperiodic 48 component, which contributes power across all frequencies. In this work, we investigate whether 49 band ratio measures reflect power differences between two oscillations, as intended. We examine 50 to what extent ratios may instead reflect other periodic changes—such as in center frequency or 51 bandwidth—and/or aperiodic activity. We test this first in simulation, exploring how band ratio 52 measures relate to changes in multiple spectral features. In simulation, we show how multiple 53 periodic and aperiodic features affect band ratio measures. We then validate these findings in a 54 large electroencephalography (EEG) dataset, comparing band ratio measures to parameterizations 55 of power spectral features. In EEG, we find that multiple disparate features influence ratio measures. 56 For example, the commonly applied theta / beta ratio is most reflective of differences in aperiodic 57 activity, and not oscillatory theta or beta power. Collectively, we show how periodic and aperiodic 58 features can drive the same observed changes in band ratio measures. Our results demonstrate how 59 ratio measures reflect different features in different contexts, inconsistent with their typical 60 interpretations. We conclude that band ratio measures are non-specific, conflating multiple possible underlying spectral changes. Explicit parameterization of neural power spectra is better able to 61 62 provide measurement specificity, elucidating which components of the data change in what ways, 63 allowing for more appropriate physiological interpretations.

64

65 **Keywords**

67 neural oscillations, frequency band ratios, spectral power ratios, theta / beta ratio, theta / alpha 68 ratio, alpha / beta ratio, electroencephalography, 1/f activity, aperiodic neural activity

69

70 Abbreviations

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EEG: electroencephalography; MEG: magnetoencephalography; ECoG: electrocorticography; LFP:
 local field potential; TBR: theta / beta ratio; TAR: theta / alpha ratio; ABR: alpha / beta ratio; CF:
 center frequency; PW: power; BW: bandwidth; EXP: aperiodic exponent; ADHD: attention-deficit

- 75 hyperactivity disorder
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77 78	Materials Descriptions & Availability Statements						
78 79 80	Project Repository						
80 81 82 83	This project is also made openly available through an online project repository in which the code and data are made available, with step-by-step guides through the analyses.						
83 84 85	Project Repository:	http://github.com/voytekresearch/BandRatios					
85 86 87	Datasets						
87 88 89	This project uses simulated data, literature text mining data, and electroencephalography data.						
89 90	Simulated Data						
91	The simulations used in this project are created with openly available software packages.						
92	Settings and code to re-generate simulated data is available with the open-access code for the						
93 94 95	project. Copies of the simulated data that were used in this investigation are available in the project repository.						
95 96	Literature Data						
97	Literature data for this project was collected from the PubMed database. Exact search terms						
98 00	used to collect the data are available in the project repository. The exact data collected from the						
99 100		e collection are saved and available in the project repository.					
101	EEG Data						
102 103	The EEG data used in this project is from the openly available dataset, the 'Multimodal Resource for Studying Information processing in the Developing Brain' (MIPDB) database. This						
105		the Childmind Institute. This dataset was released and is re-used					
105	here under the terms of the Creative Commons-Attribution-Non-Commercial-Share-Alike License						
106 107	(CC-BY-NC-SA), and is described in (Langer et al., 2017).						
108	Child Mind Institute:	https://childmind.org					
109	Data Portal:	http://fcon 1000.projects.nitrc.org/indi/cmi eeg/					
110	a (;						
111 112	Software						
113	Code used and written for this project was written in the Python programming language. All the						
114 115 116	code used within this project is deposited in the project repository and is made openly available and licensed for re-use.						
117	As well as standard library Python	, this project uses 3 rd party software packages <i>numpy</i> and <i>pandas</i>					
118	for data management, scipy for data processing, matplotlib and seaborn for data visualization and						
119 120	MNE for managing and pre-processing data.						
121 122	This project also uses open-source	e Python packages developed and released by the authors:					
123	· · ·	arameterization were done using the FOOOF toolbox.					
124	Code Repository:	https://github.com/fooof-tools/fooof					
125 126	Literature collection and analyses were done using the LISC toolbox. Code Repository: <u>https://github.com/lisc-tools/lisc</u>						
120	code Repository.						

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128 Introduction

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1301.1 History & Introduction of Band Ratio Measures131

132 Studies in cognitive and clinical neuroscience employ a broad range of analyses that are 133 designed to measure how electrophysiological measures vary with, and potentially predict, features 134 of interest such as behavioral outputs and disease states. Many such analyses focus on putative 135 rhythmic, or oscillatory, activity, organized into distinct frequency bands such as theta, alpha and 136 beta, that will collectively be referred to as 'periodic' activity. One such analysis method is to 137 calculate the ratio of power between two of these pre-specified frequency bands. For example, the 138 theta / beta ratio is calculated as the average power in the theta band, typically 4-8 Hz, divided by 139 the average power in the beta band, typically within the range of 13-30 Hz. Such measures can be 140 applied to electroencephalography (EEG), magnetoencephalography (MEG), electrocorticography 141 (ECoG) and/or local field potential (LFP) data and have been argued to be a biomarker for a variety 142 of cognitive correlates (for example, attentional control: Angelidis, van der Does, Schakel, & 143 Putman, 2016), and clinical disorders (for example, ADHD: Arns, Conners, & Kraemer, 2013; or 144 Alzheimer's: Cassani, Estarellas, San-Martin, Fraga, & Falk, 2018).

145

146 An early example of such an approach was to measure, from the correllelogram of EEG data, 147 the ratio of the dominant rhythm to the 'background' activity (Daniel, 1964). This measure was 148 developed to leverage emerging tools for spectral analysis to quantify electrophysiological features 149 of interest and integrate computational approaches, in what would later come to be referred to as 150 'quantitative EEG' or 'gEEG'. As spectral power estimation procedures became more common, 151 studies began using frequency band ratios calculated directly from estimations of band powers 152 extracted from power spectra, such as the ratio of theta to alpha power (Matoušek, 1968), which is 153 now the standard approach for calculating frequency band ratio measures (see Figure 1A).

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155 Early work used band ratio measures because they were found to be more stable than either 156 absolute or relative measures of individual frequency band powers (Daniel, 1964; Matoušek, 1968). 157 Relative power measures, including band ratios, are also used as a data normalization method, to 158 control for potential differences in confounds such as skull thickness and volume conduction, that 159 otherwise make absolute measures difficult to compare and interpret across individuals. Several 160 investigations also reported correlated changes between frequency bands, such as a frequency 161 'slowing', whereby low frequency power increases and high frequency power decreases, and 162 therefore recommended frequency band ratio measures as an ideal measure to capture such 163 changes (Lubar, 1991).

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1.2 – Applications of Band Ratio Measures

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167 In cognitive neuroscience, band ratio measures are often used in EEG studies investigating 168 possible physiological correlates of behaviors of interest, including investigations exploring 169 vigilance and alertness (Matoušek & Petersén, 1983), cognitive development and aging (Clarke et 170 al., 2001), reward processing (Schutter & Van Honk, 2005), and affect (Putman et al., 2010). One of 171 the most consistent lines of research in this area focuses on the theta / beta ratio as a potential 172 biomarker for executive function, and in particular attentional processing (Angelidis et al., 2016;

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Gordon et al., 2018; Lubar, 1991), with recent reports investigating, for example, cognitive control (Angelidis et al., 2018), and attentional control (van Son et al., 2019). Other work using EEG experiments have explored ratio measures in learning and memory, examining, for example, short term memory using the theta / beta ratio (Trammell et al., 2017), and memory impairment using the theta / gamma ratio (Moretti et al., 2009). Similar work in animals has investigated the theta / delta ratio in hippocampal recordings during associative learning paradigms in rabbits (Nokia et al., 2008) and rats (Kim et al., 2016).

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181 Frequency band ratio measures have also been used to explore changes within and between 182 individuals in contexts such as state mapping and sleep scoring, and work in development and 183 aging. In developmental work, ratio measures have been included in investigations of age related 184 electrophysiological changes (Clarke et al., 2001; Gasser et al., 1988; Matoušek & Petersén, 1973). 185 Several proposed approaches for automated sleep stage classification have also used band ratio 186 measures and found them to be useful measures (Costa-Miserachs et al., 2003; Krakovská & 187 Mezeiová, 2011; Reed et al., 2017; van Luijtelaar & Coenen, 1984). This includes work using the 188 theta / delta ratio for sleep scoring of hippocampal local field data in rats (Costa-Miserachs et al., 189 2003; van Luijtelaar & Coenen, 1984), and delta / beta ratio for human data analysis, including EEG 190 (Krakovská & Mezeiová, 2011) and ECoG (Reed et al., 2017).

192 In clinical neuroscience, band ratios are also a common approach, including in studies 193 seeking biomarkers for diagnosis, clinical monitoring, and potential intervention. Investigations into 194 the potential clinical utility of band ratio measure include investigations of anesthesia (Long et al., 195 1989), disorders of consciousness (Pfurtscheller et al., 1986), multiple sclerosis (Keune et al., 2017), 196 cerebral ischemia (Sheorajpanday et al., 2009), and Parkinson's disease (Geraedts et al., 2018). In 197 psychiatry, band ratios measures have been applied in studies of autism (Wang et al., 2016) and as 198 a potential biomarker for psychotic disorders (Howells et al., 2018). Band ratios are also commonly 199 investigated in the search for biomarkers for mild-cognitive impairment, dementia, and Alzheimer's 200 (Bennys et al., 2001; Moretti et al., 2013; Penttilä et al., 1985), recently reviewed in (Cassani et al., 201 2018).

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203 The most common clinical application of band ratios measures is in investigations of 204 attention-deficit hyperactivity disorder (ADHD) (Loo & Makeig, 2012). After early work reported a 205 relative increase in theta and decrease in beta in ADHD, theta / beta ratios were proposed as a 206 potential biomarker for the disorder (Lubar, 1991), which prompted a large number of studies 207 investigating the theta / beta ratio as a descriptive feature and potential diagnostic biomarker for 208 ADHD (see reviews in Arns, Conners, & Kraemer, 2013 & Snyder & Hall, 2006). Initial work was very 209 promising with an early meta-analysis supporting that theta / beta ratios may be a predictive marker 210 of ADHD, reporting a pooled effect size of 3.08 (Snyder & Hall, 2006). However, a more recent 211 review found much weaker support for this conclusion, also reporting that the effect size of theta / 212 beta ratios differentiating between ADHD and control groups has been decreasing across time 213 (Arns et al., 2013). Notably, the theta / beta ratio has been investigated as a potential diagnostic 214 marker of ADHD (Snyder et al., 2015), and although this led to approval by the Food and Drug 215 Administration of the United States, inconsistent evidence regarding the efficacy of using the theta 216 / beta ratio in diagnostic practice has led to a practice advisory against using it (Gloss et al., 2016). 217

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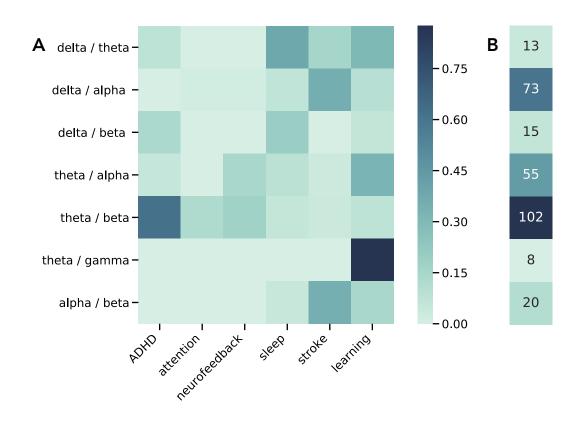


Figure 1. Literature Analysis of Band Ratio Related Articles. A) Associations between published journal articles referring to band ratio measures and cognitive and clinical associations. Each cell represents the proportion of articles referring to a specified band ratio measure that also mentions the corresponding association term. B) Total counts of the number of articles mentioning each band ratio measure.

As well as being used in investigations seeking diagnostic biomarkers, band ratio measures are commonly targeted in neurofeedback paradigms. This includes clinical applications using protocols aimed at manipulating theta / beta ratio for the treatment of ADHD (Arns et al., 2014), and as potential treatments for disorders such as autism (Wang et al., 2016). Non-clinically related neurofeedback protocols using band ratio measures have also been explored, including investigations aimed at manipulating and improving attentional and executive functions (Studer et al., 2014; Vernon et al., 2003) and relaxation (Egner et al., 2002; Raymond et al., 2005).

226 Collectively, band ratio measures are used across basic, clinical, and applied neuroscience 227 to examine a wide variety of their correlates. To explore the breadth of reported band ratio 228 correlations, we also ran an automated literature search that collects information on the number of 229 published articles that reference each ratio term and their major associates (Figure 1). This analysis 230 shows that theta / beta ratio measures are the most common, though a variety of other band ratios 231 are commonly applied, with distinct applications. We find over 250 articles that mention band ratio 232 measures, supporting that these are a relatively common method to apply to electrophysiological 233 data, across a wide range of applications. This is also likely an underestimate, as our text-mining 234 approach is limited to specific phrases that appear only in article abstracts.

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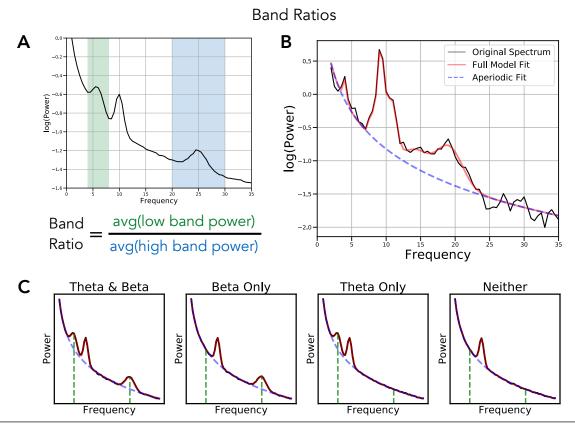


Figure 2. Overview of Band Ratio Measures and Spectral Parameters. A) An example power spectrum in which shaded regions reflect the theta (4-8 Hz) and beta band (20-30 Hz) respectively. Band ratio measures, such as the theta / beta ratio are taken by dividing the average power between these two bands. B) An example of a parameterized power spectrum, in which aperiodic activity is separated from measured periodic components. C) Examples of simulated power spectra with and without component oscillations of the theta / beta ratio. Black lines indicate the simulated data, with red line reflecting the model fit, the dashed blue line indicating the aperiodic component of the model fit, and the green lines indicating the location of canonical theta and beta oscillations. Band ratio measures, though intended to measure periodic activity, will reflect power at the pre-determined frequencies regardless of whether there is evidence of periodic activity at these frequencies.

236 **1.3 – Methodological Properties & Interpretations of Band Ratio Measures**

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Given the popularity of band ratios across domains, and their reported clinical utility, it is important to investigate and understand the properties and assumptions of such analyses, and how those assumptions relate to their interpretations. In this investigation we examine whether the general conception of band ratios as measures that specifically reflect periodic neural activity is well founded in the face of work showing that periodic properties of electrophysiological data are highly variable, often violating the assumptions of predefined frequency bands, and that they co-exist with variable and dynamic aperiodic activity (Haller et al., 2018).

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246 Methodologically, studies using band ratios typically follow a stereotyped procedure 247 whereby power in pre-defined, fixed frequency bands are calculated, from which a ratio is 248 calculated. Band ratios are typically calculated from absolute power values, though some studies 249 use relative or normalized power measures in which the power within a band is normalized by total

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power. Because ratios typically display a non-normal, skewed distribution, they are often logtransformed before further analysis.

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253 This ratio measure is then used as an electrophysiological marker that is then either analyzed 254 for potential correlations with features of interest, and/or used as a target in neurofeedback 255 paradigms. Band ratio measures are often conceptualized as capturing the proportion of a 'slower' 256 frequency band relative to some 'faster' one, and are often interpreted as a relative 'slowing' of 257 neural activity (eq: Monastra, Lubar, & Linden, 2001; Poza, Hornero, Abásolo, Fernández, & Mayo, 258 2008) or as a shift of power from one band to another (eg: Gasser, Verleger, Bächer, & Sroka, 1988), 259 which conceptualize one process explaining a change in periodic activity. Other interpretations 260 focus on interpreting and investigating ratio measures more in terms of changes within the 261 component bands, for example interpreting a decrease in theta / beta ratio as changes in the theta 262 or beta band (eg: Clarke et al., 2013), which conceptualizes one or more distinct changes in periodic 263 bands. Differences in these such interpretations include whether ratio measures are conceptualized 264 to reflect one change of reapportioning activity, or potentially multiple changes in distinct bands.

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266 What is common across these conceptualizations is that they interpret ratio measures as 267 reflecting periodic power, and so presume, as many investigations do, that pre-specified frequency 268 bands specifically measure periodic oscillatory activity. For this assumption to be valid, defined 269 frequency bands of interest, for example, 4-8 Hz theta, must capture periodic activity that is to be 270 considered as relating to that band. A known problem with applying predefined frequency bands 271 uniformly across all participants is that variation in center frequencies can lead to misestimations of 272 the desired features. This can be an underestimation, if frequency variation causes band power to 273 'move' outside the canonical range, or an overestimation, if power from an adjacent frequency band 274 is captured in the examined range. Similar issues can arise if the bandwidth of frequency bands 275 violates expectations and/or is different between groups. These potential periodic confounds 276 challenge the assumption that band ratio measures relate specifically to relative periodic power (see 277 Figure 3A).

279 An example of this issue has been previously demonstrated in a sample of participants with 280 ADHD, whereby an increased theta / beta ratio, as measured using canonical band definitions, was 281 found to actually reflect a slowed alpha peak in the ADHD group (Lansbergen et al., 2011). In this 282 case, the theta / beta ratio calculated using individualized frequency bands found no difference 283 between groups. This suggests that, in at least some cases, frequency variation can lead to 284 measurements and interpretations of band ratios that do not accurately reflect the actual properties 285 of the data. This has led to suggestions that band ratios measure should be computed using 286 individualized frequency bands (Saad et al., 2018).

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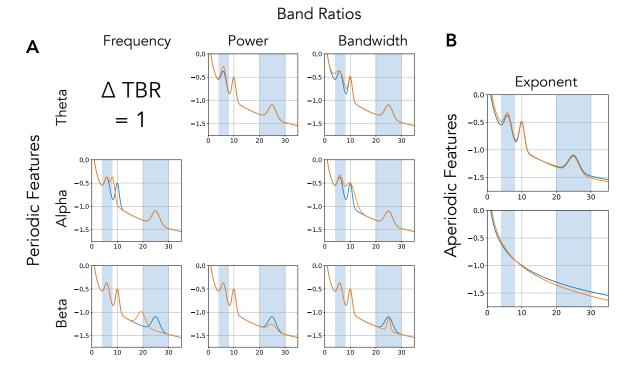


Figure 3. Equivalent Band Ratio Differences from Distinct Changes. Simulations demonstrating the underdetermined nature of band ratio measures. In each case, the power spectrum plotted orange has the same difference of measured theta / beta ratio from the reference spectrum, in blue. This difference in ratio can arise from changes in multiple different features of the data, including a shift in: A) the periodic properties such as the center frequency, power or bandwidth of oscillations, and/or from a shift in; B) aperiodic component of the data. Differences in aperiodic activity can induce differences in measured band ratios, even without any periodic components present.

288 Beyond the periodic confounds, a broader issue is the implicit assumption that frequency 289 definitions reflect periodic activity in the data, and that this activity can be specifically captured by 290 measuring power averaged across a frequency range. This assumption is in general invalid, as 291 electrophysiological activity includes not only periodic components, but a 1/f-like distributed 292 aperiodic component (Haller et al., 2018; B. J. He, 2014), which has power at all frequencies, but 293 does not consist of periodic activity (see Figure 2B). The presence of this 1/f-like activity, henceforth 294 referred to as the 'aperiodic component', entails that there will always be power in a given frequency 295 range, but that this power should not necessarily be assumed to reflect periodic activity. Rather, 296 power at a particular frequency, or frequency range, reflects, at least in part, aperiodic activity, and 297 only partially, if at all, reflects periodic activity. A marker that there is actual periodic power in a 298 signal is that there should be a band specific peak over and above this aperiodic component 299 (Buzsáki et al., 2013). To specifically measure this periodic component of the signal, one should 300 measure the power in this band specific peak relative to the aperiodic component of the signal 301 (Haller et al., 2018).

Band ratio measures, as currently applied, do not address the confound of ubiquitous aperiodic activity in neural signals. Aperiodic neural activity is known to be variable both within (Podvalny et al., 2015) and between individuals (Voytek et al., 2015). This variability raises the possibility that band ratio measures may reflect, at least partially, aperiodic activity and that

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307 measured differences within and between individuals may be driven by differences in aperiodic 308 properties of the data (see Figure 3B). The very observation that there are correlated changes across 309 frequency bands that helped popularize band ratio measures (Lubar, 1991) can even be interpreted 310 to support the suggestion that a parsimonious description of the data could be changes in aperiodic 311 properties, across all frequencies. This is also broadly consistent with the interpretations of ratios 312 reflecting 'substitutions' of power between bands (Gasser et al., 1988) in the sense that one process 313 explains the changes across different frequency regions (though inconsistent with this being a shift 314 of periodic activity).

315

316 In summary, band ratio measures are a common analyses measure that are calculated across 317 two frequency bands that are designed to, and are interpreted as, reflecting relative periodic 318 activity. However, even when oscillations are clearly present, variations in the measure may reflect 319 not only the power across the two bands, but may be driven by differences in the center frequencies, 320 and/or the bandwidths of such periodic components and, can also be driven by changes in 321 aperiodic activity with or without periodic activity being present (see Figure 2C). Altogether, this 322 suggests that band ratio measures are underdetermined, whereby a change in one or many 323 different features of the data may drive analogous differences in band ratio measures (Figure 3). If 324 so, not only are typically interpretations of band ratio measures unsupported, but band ratio 325 measures, by themselves, may be essentially uninterpretable, as underlying physiological causes of 326 changes in the measure are undecipherable from the measure itself, but reflect different properties 327 of the data.

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329 To investigate these issues, we examine the properties and validity of band ratio measures, 330 including, 1) how are band ratio measures influenced by different features of periodic activity, 331 including center frequency, power and bandwidth, and 2) how band ratio measures are influenced 332 by changes in aperiodic properties of the data, including the aperiodic exponent and offset. We 333 start by systematically exploring the properties of band ratio measures across simulated data that 334 mimic the statistics of real data, for which ground truth is known. We use these simulations to 335 evaluate how changes in different features, and their combinations, influence band ratio measures. 336 We follow by analyzing a large EEG dataset (n = 126) in which we applied band ratio measures and 337 compared ratios to methods that explicitly parameterize periodic and aperiodic features of the data, 338 to infer which neural features influence and contribute to band ratio measures. We find that many 339 different features of the data can give rise to band ratio differences, making them effectively 340 uninterpretable in isolation, without additional context of the rest of the power spectral features 341 involved. Therefore, we conclude that band ratios should not be interpreted as a well-posed 342 method to specifically measure periodic properties of neural times series, and comment on how the 343 methodological findings from this work can be used to interpret prior work, and what it suggests 344 for future investigations.

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346 Methods

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348 In order to investigate the properties of frequency band ratios, we explored calculating band 349 ratio measures across simulated power spectra, for which ground truth values were known, as well 350 as investigating their application in EEG data. As a comparison to the band ratio measures, periodic 351 (oscillatory) and aperiodic properties of power spectra were characterized using the fitting-352 oscillations-&-one-over-f (FOOOF) toolbox (Haller et al., 2018). Band ratio measures were 353 compared to the outputs of the parameterization of the power spectra, which quantifies the center 354 frequency (CF), power (PW) and bandwidth (BW) of identified periodic components, as well as the 355 exponent and offset (described below) of the aperiodic component. Using these parameterizations, 356 we evaluate which components of the data the band ratio measures reflect. For all analyses, 357 canonical frequency band definitions were defined as: theta (4-8 Hz), alpha (8-13 Hz), beta (13-30 358 Hz).

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Analyses were done using Python (version 3.7), including common libraries numpy, pandas, scipy, matplotlib and seaborn for analysis and visualization. The MNE library was used for managing and processing EEG data (Gramfort et al., 2014). Custom code was used to calculate band ratio measures and perform analyses. All code for this project is available in the project repository (<u>https://github.com/voytekresearch/BandRatios</u>).

- 366 **2.1 Literature Analysis**
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368 The literature analysis was done use the 'Literature Scanner' (LISC) Python toolbox 369 (Donoghue, 2019). Briefly, this toolbox allows for collecting and analyzing literature data by curating 370 search terms of interest, gathering related articles from available databases, and analyzing the 371 results. For this analysis, a list of band ratio terms (e.g., "theta / beta ratio") and related association 372 terms (e.g., "attention"), with relevant synonyms and exclusion words, was manually curated. 373 Searches were performed to determine the number of articles in the PubMed database that 374 reference these terms in their abstract, and the number of co-occurrences of band ratio terms with 375 association terms. Association scores were calculated as the proportion of articles referencing a 376 band ratio measure that also mention one of the included association terms.

- 378 2.2 Simulations
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380 Neural power spectra were simulated to match the statistics of electrophysiological neural 381 data, by combining a 1/f-like aperiodic component with overlying peaks of periodic activity, with 382 overlying noise (Haller et al., 2018). The aperiodic component describes the 1/f-like characteristic 383 of neural power spectra and is entirely described by the aperiodic 'exponent' and 'offset.' The aperiodic exponent, meaning the χ in $\frac{1}{f\chi}$, describes the steepness of the 1/f, and the 'offset,' 384 describes the vertical translation of the aperiodic activity. Periodic components describe putative 385 386 oscillations which display power above the aperiodic component. Periodic components are simulated as Gaussians, and are described by a 'center frequency' (CF) in hertz, 'power' (PW) from 387 388 the aperiodic component to the oscillatory peak in arbitrary units (au), and 'bandwidth' (BW) which 389 describes the width of the peak, also measured in hertz. The simulation ultimately follows:

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 $P = L + \sum G_n$ 391 in which L is the aperiodic component, described as

$$L = 10^b * \frac{1}{f}$$

in which b is the offset and χ is the exponent. On top of this, periodic components are added with 393 394 each of *n* peaks described as a Gaussian, as:

 $G_n = a * \exp(\frac{-(F-c)^2}{2 * w^2})$ 395

396 in which c is the peak center frequency, and a and w are the height and width of the gaussian, 397 equivalent to the power and bandwidth of the peak.

399 Spectra were simulated for the frequency range of 1-35 Hz, with a 0.5 Hz frequency 400 resolution. Default aperiodic and periodic parameter values were chosen to capture physiologically 401 realistic values. A small amount of normally distributed noise (0.005 au) was added to all spectra to 402 emulate real power spectra.

404 We calculated band ratios from simulated power spectra by dividing mean power across the 405 low band range by the mean power across a high band range. We calculated the theta / beta ratio, 406 theta / alpha ratio, and alpha / beta ratio.

408 To measure how spectral parameters relate to band ratio measures, spectra were simulated 409 where a single parameter was varied across a range while the remaining parameters were kept at 410 their default values. From these spectra the theta / beta, theta / alpha and alpha / beta ratios were 411 calculated to track how individual parameters affect ratio measures. Since CF, PW, and BW are 412 specific to a peak, they were all individually varied for both low-band and high-band peaks. The 413 ranges of values for each parameter are given in supplemental tables 1 & 2.

414

415 We then studied how band ratio measures are affected by multiple interacting changes in 416 spectral parameters. Further simulations were carried out as two parameters from the set {CF, PW, 417 BW, EXP} were simultaneously varied across their respective ranges. All combinations of paired 418 parameter simulations were calculated and analyzed. The default parameter settings and ranges 419 remained the same as the single parameter simulations.

421 2.3 EEG Data Analysis

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423 To study how various spectral parameters affect band ratio measures, we used the openly 424 available 'Multimodal Resource for Studying Information Processing in the Developing Brain', or 425 MIPDB, dataset of human EEG data released by the Child Mind Institute (Langer et al., 2017). The 426 study population is a community sample of children and adults (n = 126, age range = 6-44, age 427 mean = 15.79, age standard deviation = 8.03, number of males = 69). Data for each subject includes 428 resting state and task EEG data, behavioral measures, and eye tracking data. For the current 429 investigation, we analyzed eyes-closed resting state data, collected on a 128 channel Geodesic 430 Hydrocel system. Of the 126 participants in the dataset, 9 did not include resting state data 431 collection, as indicated by the dataset description, and were therefore excluded. In addition, a 432 further 6 participants were excluded from this analysis due to missing the resting state recording

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file (1 subject) or not having enough resting data events to analyze (5 participants) leaving 111participants included in the final analysis.

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436 In the resting state protocol, participants were instructed to fixate on a central cross, and 437 open or close their eyes when they heard a beep, alternating between 20 second blocks of eyes 438 open and 40 second blocks of eyes closed. The dataset includes a pre-processed and artifact 439 corrected copy of the data, which was used here, with full details of the pre-processing described 440 in (Langer et al., 2017). Briefly, bad electrodes were identified and interpolated, eye artifacts were 441 regressed out of the EEG from EOG electrodes, and a PCA approach was used to remove sparse 442 noise from the data. We further identified flat channels (channels with no data) and interpolated 443 them, and re-referenced data to a common average reference.

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For the current analyses, we used the eyes closed resting state data, and extracted the time period of 5 – 35 seconds within the 40 second eyes closed resting segments, excluding the 5 seconds post and prior to eye opening. We used the first block for each participant for analysis. Power spectra were calculated for each channel using Welch's method, using 2 second windows with 25% overlap.

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451 We then parameterized the calculated power spectra to return estimates of periodic and 452 aperiodic parameters. The model parameterization we used is agnostic to frequency bands, fitting peaks wherever they're found in the frequency spectrum regardless of canonical band definitions 453 454 (Haller et al., 2018). We determined that activity was contained in a band if the peak of an oscillation 455 was contained in our aforementioned band definitions. Settings for parameterizing power spectra 456 are as follows: the width for a detected peak was bound between 1 - 8 Hz, with a maximum number 457 of detectable peaks set at 8, a minimum threshold for detecting a peak set at 0.1 au, the threshold 458 for detecting was set at the default value of 2 standard deviations above the noise floor, and spectra 459 were fit in 'fixed' mode without a knee.

460

For all band ratio measures, we calculated Spearman correlations between spectral parameters, including center frequency, power and bandwidth of each oscillation band, as well as the aperiodic exponent, across all channels. We do not report correlations to aperiodic offset, as offset shifts by themselves do not affect ratio measures (see simulation results). In addition, we calculated Spearman correlations between each ratio measure and participants' ages, and between spectral parameters and age.

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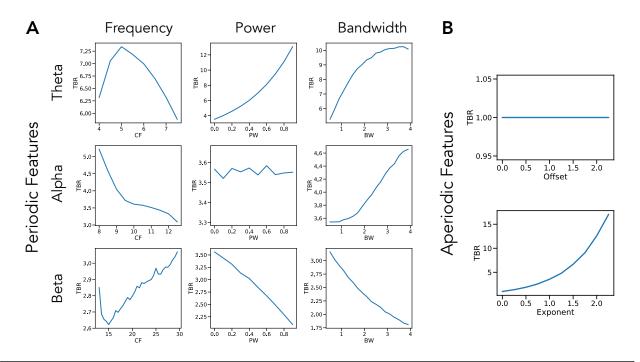


Figure 4. Single Parameter Simulations. Simulations of changes in measured theta / beta ratio as individual parameters are varied, including: A) periodic parameters and B) aperiodic parameters. Changes in theta center frequency show an increase in theta / beta ratio as the heightened activity is better captured in the canonical band, then decreases as activity leaves the band. Increasing theta power and bandwidth both increase TBR while increasing beta power and bandwidth decreases theta / beta ratio. The center frequency and bandwidth of alpha peaks also influences measured theta / beta ratio, even though alpha is not supposed to be included in the measure. Beta parameters essentially have the inverse effect of changes in theta parameters. Changes in aperiodic exponent also substantially impact measured theta / beta ratio.

468 **Results**

469

470 **3.1 Simulation Results**

471

472 We started by investigating, in simulation, the extent to which band ratios capture periodic 473 power as typically interpreted, and/or to what extent they are potentially related to other periodic 474 or aperiodic spectral parameters. Measured theta / beta ratios across simulations in which one 475 spectral parameter was changed at a time, are reported in Figure 4. As expected, when examining 476 periodic changes (Figure 4A) the theta / beta ratio is strongly driven by power of theta and beta 477 oscillations. However, ratio measures can also be influenced by the center frequency and bandwidth 478 of the theta and beta peaks. We also replicate previous work showing that the center frequency of 479 the alpha peak can impact measures of theta / beta ratio, (Lansbergen et al., 2011), and extend this 480 to include alpha bandwidth. For aperiodic changes (Figure 4B), we see that the aperiodic exponent 481 has a significant effect on measured ratio values.

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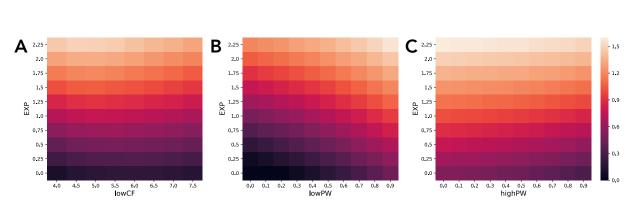


Figure 5. Interacting Parameter Simulations. Measured theta / beta ratio values in simulations as two spectral parameters are varied together. Ratio measures plotted in log10 space due to their skewed distributions. Combinations plotted are aperiodic exponent with low band center frequency (A), as well as with low band power (B) and high band power (C). All combinations of varying parameters influence measured band ratio values.

Collectively, we see that a wide range of different parameter changes can affect measured ratios. In this case, 8 of the 10 parameters alter theta / beta band ratio, with the only exceptions being the aperiodic offset, which changes power equally between ratio bands, and power in the non-included band, in this case alpha (for the theta / beta ratio). Of note, however, is that the scale of this effects can be quite different, with the power of the included bands and the aperiodic exponent having the biggest impacts. The findings for other band ratio measures are consistent with those for the theta / beta ratio, with full results for them available in the project repository.

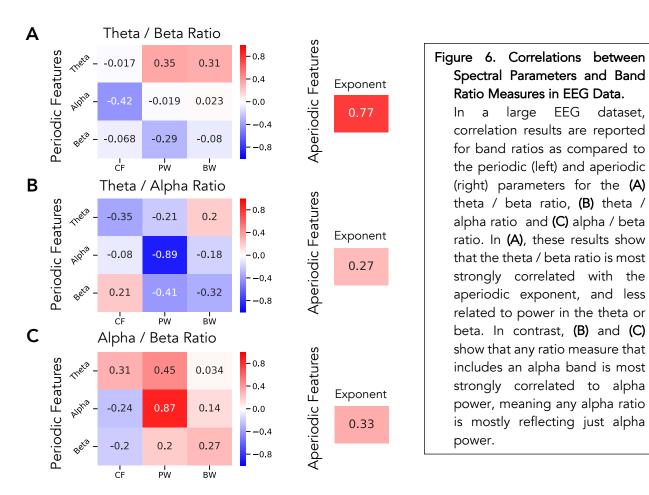
491 We further explored simulations of pairwise combinations of parameter changes, to 492 investigate how ratio measures are affected by concomitant changes in multiple parameters (Figure 493 5). These simulations include, for example, measured theta / beta band ratios as the aperiodic 494 exponent and theta center frequency both vary, showing an interaction between them (Figure 5A). 495 We can see how changes in aperiodic exponent interact with power changes in the lower (Figure 496 5B) and higher (Figure 5C) bands. These simulations also demonstrate that both features have an 497 impact on measured ratios, and allow a comparison of scale, showing, for example, that although 498 the influence of low band power and aperiodic exponent is of a similar magnitude, when compared 499 to high band power, the effect of aperiodic exponent changes is relatively much larger. Collectively, 500 through these simulations, we see that changes in different spectral parameters can interact and 501 drive different patterns of differences in measured band ratios. Further simulations of interacting 502 parameters across all other combinations are available in the project repository.

503

504 **3.2 EEG Data Results**505

506 We continue our investigation with EEG data recorded during resting state, and compare 507 band ratio measures to parameterized power spectral features. For all correlations here, we report 508 results across all channels. Re-running these analyses with channel groups, using frontal, central,

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509 and parietal sub-selections showed qualitatively similar patterns, the results of which are available 510 in the project repository.

511

For the theta / beta ratio, within periodic spectral parameters we find, as expected, that the strongest relationship is between theta / beta ratio and theta power (r = 0.35, p < 0.001) with a similarly high correlation with beta power (r = -0.29, p < 0.01). However, when considering aperiodic parameters, we find a much stronger relationship between theta / beta ratio and aperiodic exponent (r = 0.77, $p < 10^{-20}$). The full set of spectral parameter correlations is available in Figure 6A.

517

In contrast, for the theta / alpha ratio, the highest correlation across both periodic and aperiodic spectral parameters was for alpha power (r = -0.89, $p < 10^{-35}$), with a much lower correlation with aperiodic exponent (r = 0.27, p < 0.01). This pattern of correlations was also similar for the alpha / beta ratio, with a strong correlation with alpha (r = 0.87, $p < 10^{-30}$), and a much weaker one with aperiodic exponent (r = 0.33, p < 0.001). Spectral parameter correlations for the theta / alpha ratio and alpha / beta ratio are available in Figure 6B & 6C respectively.

524

525 We also calculated average ratio measures and spectral parameters for each channel, across 526 the group. Topographies of these measures are plotted in Figure 7. Here we can see, for example, 527 that the spatial topography of the theta / beta ratio is most similar to that of the aperiodic exponent, 528 with a strong spatial correlation (r = 0.77, $p < 10^{-20}$). The topography of alpha / beta ratio is nearly

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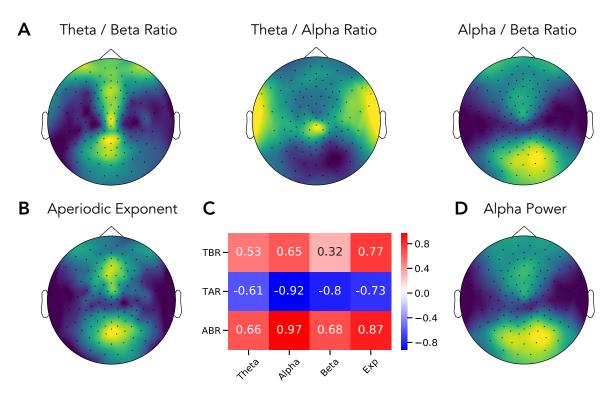


Figure 7. Topographies of Band Ratio Measures and Spectral Parameters. Topographical maps of the A) ratios measures, including the theta / beta ratio, theta / alpha ratio and alpha / beta ratio. For comparison, the topography of the aperiodic exponent (B) and of alpha power (D) are also presented. Each topography is scaled to relative range of the data, with higher values plotted in lighter colors (yellow). C) The spatial correlation between topographies of each ratio measure to spectral parameters including power of theta, alpha and beta, and the aperiodic exponent.

529 identical to the topography of alpha power (r = 0.97, $p < 10^{-70}$), with a strong inverse relation 530 between the theta / alpha ratio and alpha power (r = -0.92, $p < 10^{-45}$).

531

532 We also calculated how each measure correlated with age. The theta / beta ratio was found to be highly correlated with age (r = .67, $p < 10^{-15}$), with the negative correlation indicating that 533 534 older adults have higher theta / beta ratios. In comparison, the theta / alpha ratio had a much 535 smaller correlation with age (r = -0.37, p = 0.0001) and the alpha / beta ratio was not significantly 536 correlated with age (r = -0.12, p = 0.22). For spectral parameters, the aperiodic exponent was found to be highly correlated with age (r = 0.68, $p < 10^{-15}$), consistent with previous reports (W. He et al., 537 538 2019; Voytek et al., 2015).

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540 **Discussion**

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543

542 4.1 Methodological Discussion Points

544 Through investigations of both simulated and real data, we find that frequency band ratio 545 measures, though typically applied and interpreted as reflecting the relative periodic power of 546 distinct frequency bands, can actually reflect a large number of distinct changes in the underlying 547 data. These band ratio measures therefore capture multiple different changes in periodic and aperiodic properties. Part of this stems from the use of predefined frequency bands of interest, as 548 549 has been previously reported (Lansbergen et al., 2011; Saad et al., 2018). Here, we replicate and 550 extend this finding, showing how center frequency, and also oscillatory bandwidth, can influence 551 band ratio measures in ways that can be misinterpreted as reflecting power differences. In addition, 552 we show how frequency band ratio measures may commonly capture, at least partially, aperiodic 553 components of electrophysiological data.

554

555 Specifically, we used a parameterization model conceiving of the power spectrum as the 556 combination of an aperiodic, 1/f-like spectrum, characterized by an offset and exponent, with 557 overlying periodic 'peaks', each characterized by a center frequency, power (over and above the 558 aperiodic background) and bandwidth measure. With this approach, we show many of these 559 parameters can similarly affect band ratio measures in simulation. When applied to real data, we 560 find that different parameters do affect ratio measures, with different patterns for different ratio 561 measures. For example, theta / beta ratio measures mostly reflect aperiodic exponent, whereas 562 theta / alpha and alpha / beta ratios mostly reflect alpha power. In no ratio measures did we find 563 evidence that the measure primarily reflects power within both specified bands.

565 Given the underdetermined nature of band ratio measures in the face of multiple features 566 of the data that may be changing, we conclude that band ratio measures are not an appropriate 567 measure for characterizing electrophysiological data, at least not in isolation. This is because are 568 uninterpretable in terms of knowing which component(s) of the data they actually reflect. Therefore, we recommend complementary or alternate approaches. These include methods that fully 569 570 parameterize neural power spectra, specifically measuring periodic and aperiodic components 571 (Haller et al., 2018), which allows for precise quantification of which features of the data vary within 572 and between individuals.

573

564

574 A prior recommendation, that attempts to address center frequency differences (Lansbergen 575 et al., 2011), is that band ratio measures should use individualized frequency bands (Saad et al., 576 2018). It should be noted that the recommended approach, originally proposed by (Klimesch, 577 1999), is to use individualized bands based on an alpha band anchor point, whereby theta and beta 578 can be defined as below and above the observed alpha peak. Though this addresses some issues 579 with varying alpha center frequency, it does not specifically establish if there is a defined theta or 580 beta peak, over and above aperiodic power, nor does it identify specific center frequencies should 581 such periodic activity be present. Because this approach also does not separate aperiodic from 582 periodic power, individualized peak detection, especially when anchored to alpha peaks, is 583 insufficient to address the problems highlighted here.

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585 It has previously been reported that ratio measures are stable and have high test-retest 586 reliability within individuals (Angelidis et al., 2016; Monastra et al., 2001; Ohlund, 2000). This is not 587 necessarily in conflict with the finding here that band ratio measures may reflect many distinct 588 features of the data; stable test-retest reliability merely suggests that whichever feature(s) are 589 captured by band ratios within a given subject are themselves stable. However, that band ratios 590 across individuals, and in particular across different populations, may reflect different properties of 591 the data may well help explain why there has been difficulty in reproducing several findings using 592 band ratios. For example, recent failures to replicate band ratio measures include follow ups on 593 previously reported relations with trait anxiety (van Son et al., 2018) or attentional control (van Son 594 et al., 2019). In clinical work, there have been inconsistent findings relating the theta / beta ratio to 595 ADHD (Liechti et al., 2013; Ogrim et al., 2012). It is possible that when investigating varying 596 populations, different features of the data may be driving different observed ratio measures, and 597 this may relate to the significant variance of band ratio measures and their correlates found across 598 studies.

599

601

600 4.2 Interpretation Related Discussion Points

602 The findings cast doubt on the interpretations of prior reports that use band ratio measures 603 and interpret them as primarily reflecting periodic power. Where such studies are reproducible, 604 recontextualization of such findings should consider multiple possible interpretations, including, for 605 example that, a) there is a true change in the power ratio of activity between distinct frequency 606 bands reflecting periodic activity, b) there is a difference in periodic parameters other than power, 607 such as in center frequency and/or bandwidth, c) band ratio measures reflect differences in 608 aperiodic activity, or, d) some combination of the above. Based on data analyzed, the theta / beta 609 ratio is most likely to reflect aperiodic activity, whereas the theta / alpha and alpha / beta ratios are 610 most likely to primarily reflect alpha power. That said, ratio measures could vary across studies in 611 what they reflect, and/or reflect interactions between parameters. Re-evaluations of prior work 612 and/or follow up investigations should seek to re-evaluate such data to investigate which features, 613 in each case, are driving the measured changes in band ratios, and update interpretations 614 accordingly.

615

616 In this investigation we replicated the consistently reported finding that band ratio measures 617 vary systematically with age (Angelidis et al., 2016; Bresnahan et al., 1999; Buyck & Wiersema, 2014; 618 Clarke et al., 2001; Gasser et al., 1988; Monastra et al., 2001; Ogrim et al., 2012; Putman et al., 619 2010), as well as the finding that aperiodic activity also varies systematically with age (Voytek et al., 620 2015). Since we also find that band ratio measures are highly correlated with aperiodic activity 621 (especially the theta / beta ratio), this is altogether consistent with the idea that the relation of band 622 ratio measures to age is plausibly due to band ratios reflecting aperiodic activity. We note that the 623 dataset used here consists of young participants, and the pattern of findings here is also consistent with recent work showing that the relation of aperiodic activity to age is also apparent in younger 624 625 participants, and that changes in aperiodic activity across age better explains developmental 626 patterns rather than previous reports of correlated changes across multiple distinct oscillation bands 627 (W. He et al., 2019).

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629 Overall, the EEG data analyzed here suggests that ratio measures, and the theta / beta ratio in particular, often largely reflects aperiodic activity. As well as the relationship of aperiodic activity 630 631 and band ratios to age, this is also consistent with other reports that previously reported correlates 632 of band ratios have also been found to relate to aperiodic activity. For example, when band ratios 633 are used in sleep scoring, it is typically done with the delta / theta ratio, which we predict likely also 634 captures aperiodic changes, which would be consistent with recent reports that aperiodic activity 635 changes systematically with sleep (Lendner et al., 2019). Collectively, these shared correlates are 636 consistent with suggestion that band ratio measures likely often reflect aperiodic activity.

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638 A key prediction, if ratio measures often reflect aperiodic properties, is that the reported 639 findings will not be specific to the frequency ranges used to measure the ratios, as aperiodic effects 640 should exist across all frequencies. Indeed, correlated change across frequency bands is one of the 641 observations that led to the popularity of band ratio measures (Lubar, 1991). It has also been 642 reported that distinct ratio measures across different frequency bands show similar patterns, for 643 example that both delta / beta and theta / beta ratios relate to cognitive correlates (Schutter & Van 644 Honk, 2005; Tortella-Feliu et al., 2014), both theta / alpha and theta / beta have been reported to 645 relate to ADHD (Barry et al., 2003), and multiple different ratios show similar patterns in investigations of Alzheimer's disease (Poza et al., 2008). In cases such as these, in which different 646 647 band ratio measures show approximately similar trends across a wide array of band pairs, a plausible 648 interpretation is that these findings do not reflect correlated changes across multiple distinct 649 frequency bands, but rather that they are all capturing frequency-agnostic aperiodic shifts. 650

651 In neurofeedback designs, where band ratios are a target for manipulation rather than a 652 descriptive measure, findings are also consistent with the possibility that targeting ratios at least 653 partially manipulates aperiodic properties, rather than targeting oscillation bands specifically. For 654 example, a recent report showed that targeting beta in a feedback design also induces changes in 655 the alpha band (Jurewicz et al., 2018), which challenges the possibility of targeting different bands 656 independently. Where investigations probe the specificity of neurofeedback protocols, non-specific 657 effects have been reported, such as an effect on beta from a theta / alpha protocol (Egner et al., 658 2004), and changes in alpha when using a theta / beta protocol (Bazanova et al., 2018; Limin Yang 659 et al., 2015), all of which is consistent with ratios reflecting aperiodic activity.

661 If a considerable proportion of the variance of band ratios measures is due to aperiodic 662 properties, and not well described or interpreted as band specific changes, then it becomes an 663 open question to ask what the physiological interpretation should be, and therefore how these 664 findings should be interpreted. One hypothesis is that the aperiodic properties of neural time series 665 may relate the relative balance of excitatory and inhibitory activity (Gao et al., 2017). Though further work is required to explore this hypothesis and how it relates to measurements done with band 666 667 ratios, this does suggest a potential link between what has been measured in band ratios, as a 668 correlate of various cognitive markers and disease states, and potential interpretations related to 669 excitation and inhibition. A more general review of aperiodic properties in neural data, sometimes 670 referred to 'scale-free' activity, is available in (B. J. He, 2014).

672 Particular attention should be paid to ratio measures applied in clinical applications, in which 673 the pursuit of biomarkers based on faulty measures could hinder, rather than ameliorate, clinical

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674 practice. For example, the findings here on ratio measures are consistent with the practice advisory 675 that using theta / beta ratio measures in the context of ADHD is not an appropriate measure (Gloss 676 et al., 2016). Rather, the prediction based on these results for ADHD would be that the oft reported 677 theta / beta correlate is likely a reflection of differences in aperiodic activity. In other work, we have 678 found exactly this: that aperiodic properties are correlated with theta / beta measures in a 679 population with ADHD, and that the aperiodic measures themselves better relate not only to 680 disease state but also to medication status (Robertson et al., 2019). For other clinical disorders that 681 have been investigated with band ratio measures, such as Alzheimer's disease (Cassani et al., 2018), 682 or psychotic disorders (Howells et al., 2018) we recommend that investigations should follow up on 683 which underlying features best explain changes in ratio measures, and update interpretations and 684 future work on biomarkers accordingly.

685

686 A notable exception, as we found in analyzed EEG data, to ratio measures reflecting 687 aperiodic shifts is in cases in which ratio measures include the alpha band. When the alpha band is 688 included in the ratio, band ratio measures tend to primarily reflect alpha power. This is likely due to 689 the prominence of the alpha band, where alpha is typically present across participants, has very 690 high power, and is dynamic. Thus, it is logical that ratio measures that include the alpha band largely 691 reflect alpha dynamics, as we observed here. This effect may also be exaggerated in our analysis, 692 as we are analyzing eyes closed data, in which alpha power is most prominent, though the pattern 693 of results is consistent when re-run on eyes open data. Investigations in which ratio measures such 694 as delta / alpha or theta / alpha are used should investigate to what extent the dominant effect they 695 are capturing is alpha dynamics. Overall we recommend that reports from studies using band ratios 696 including alpha should consider if the findings are likely to be largely explained by alpha dynamics. 697

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698 Conclusion

699

700 Frequency band ratio measures are a common analysis approach applied to neural field 701 data, including EEG, MEG, ECoG and LFP. Band ratio approaches have been applied across many 702 domains, including basic research investigating executive functions, learning and memory, and 703 sleep; in clinical investigations including investigating ADHD and dementia; and in applied work 704 leveraging them for neurofeedback applications. Though typically interpreted as a normalized 705 measure reflecting the relative power of distinct periodic components, here we show that band ratio 706 measures can reflect not only multiple features of periodic neural activity, including the center 707 frequency, power and bandwidth of periodic components, but can also be driven by variations in 708 aperiodic activity. This is demonstrated in simulation, and also in empirical work applied to a large 709 EEG dataset in which we show how multiple spectral features relate to measured band ratios, 710 making them an imprecise metric. For example, the most dominant contributor to the theta / beta 711 ratio is the aperiodic exponent, whereas the theta / alpha and alpha / beta ratio predominantly 712 reflect alpha power. Overall, band ratio measures are found to be underdetermined, and so across 713 participants, recording modalities, species, and contexts may reflect different components of the 714 signal. This makes comparisons with band ratio measures difficult, if not impossible, and questions 715 their typical interpretations as reflecting periodic activity. As an alternative, we recommend that 716 parameterization of neural power spectra is able to better capture which components of neural 717 signals vary and relate to features of interest, without conflating changes in periodic and aperiodic 718 activity, as band ratio measures do.

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965 Supplementary Materials

		Theta	Alpha	Beta
	Default	6	10	21.5
CF	Range	4 - 8	8 - 13	13 - 30
	Increment	0.25	0.25	1
	Default	0.5	0.5	0.5
PW	Range	0 - 1.0	0 - 1.0	0 - 1.0
	Increment	0.1	0.1	0.1
	Default	0.1	0.1	0.1
BW	Range	0.2 - 0.4	0.2 - 0.4	0.2 - 0.4
	Increment	0.2	0.2	0.2

Supplemental Table 1. Simulation Parameters for Periodic Components

966

	Default	Range	Increment
Offset	0	0 - 2.5	0.25
Exponent	1	0 - 3	0.2

Supplemental Table 2. Simulation Parameters for Aperiodic Components