1	Full Title: Delay-period activity in frontal, parietal, and occipital cortex tracks different
2	attractor dynamics in visual working memory
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4	Short Title: Neural correlates of attractor dynamics in visual working memory
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## 26 Abstract

27 One important neural hallmark of working memory is persistent elevated delay-period 28 activity in frontal and parietal cortex. In human fMRI, delay-period BOLD activity in frontal and 29 parietal cortex increases monotonically with memory load and asymptotes at an individual's 30 capacity. Previous work has demonstrated that frontal and parietal delay-period activity 31 correlates with the decline in behavioral memory precision observed with increasing memory 32 load. However, because memory precision can be influenced by a variety of factors, it remains 33 unclear what cognitive processes underlie persistent activity in frontal and parietal cortex. Recent 34 psychophysical work has shown that attractor dynamics bias memory representations toward a 35 few stable representations and reduce the effects of internal noise. From this perspective, 36 imprecision in memory results from both drift towards stable attractor states and random 37 diffusion. Here we asked whether delay-period BOLD activity in frontal and parietal cortex 38 might be explained, in part, by these attractor dynamics. We analyzed data from an existing 39 experiment in which subjects performed delayed recall for line orientation, at different loads, 40 during fMRI scanning. We modeled subjects' behavior using a discrete attractor model, and 41 calculated within-subject correlation between frontal and parietal delay-period activity and 42 estimated sources of memory error (drift and diffusion). We found that although increases in 43 frontal and parietal activity were associated with increases in both diffusion and drift, diffusion 44 explained the most variance in frontal and parietal delay-period activity. In comparison, a 45 subsequent whole-brain regression analysis showed that drift rather than diffusion explained the 46 most variance in delay-period activity in lateral occipital cortex. These results provide a new 47 interpretation for the function of frontal, parietal, and occipital delay-period activity in working 48 memory.

## 49 Introduction

50 Working memory – the ability to mentally retain and manipulate information to guide 51 behavior – is crucial for many aspects of high-level cognition [1-3]. One prominent neural 52 hallmark of working memory performance is persistent elevated delay-period activity in frontal 53 and parietal cortex. Specifically, blood oxygen level-dependent (BOLD) activity in frontal and 54 parietal cortex increases monotonically with memory load and asymptotes at an individual's 55 memory capacity [4, 5]. Activity in these networks is thought to reflect the engagement of 56 control [6, 7]. For example, one recent study has demonstrated that persistent activity in parietal 57 cortex tracks the demands of binding stimulus content to its trial-specific context, rather than 58 memory load per se [8]. These signals have been shown to correlate with individual memory 59 capacity [4, 5] and with memory precision [8-10]. In contrast, persistently elevated activity 60 during the delay period is often absent in occipital cortex, despite the reliable representation of 61 stimulus-specific information [8, 10-13].

Recent psychophysical work has shown that inaccuracies in working memory are due to 62 63 both random error and systematic biases. For example, when subjects remember features drawn 64 from a uniform stimulus space, their responses are not uniform. Instead, the responses "cluster" 65 around a small number of specific values [14-16]. Further modeling work has demonstrated this 66 clustering can be explained by attractor dynamics that pull memories to specific locations in 67 mnemonic space (i.e. color memories are 'attracted' to red). While this induces systematic error 68 into the memories, it also stabilizes memories near the attractors [16]. Thus, engaging attractor 69 dynamics is thought to be especially beneficial when memory load is higher, because increased 70 noise in stimulus representations can be counteracted by increasing drift towards a few stable 71 representations.

72 Because load-related imprecision in working memory performance reflects both random diffusion and drift towards stable attractor states, it remains unclear which of these dynamics 73 74 could account for load-sensitive delay-period activity in parietal and frontal cortex. In the current 75 study, we analyzed data from an existing experiment in which subjects performed delayed recall 76 for line orientation, at different memory loads, during fMRI scanning. We modeled subjects' 77 behavior using a discrete attractor model, and regressed the resultant load-sensitive estimates of 78 drift and diffusion against load-dependent delay-period activity in parietal and frontal cortex. We 79 found that an increase in frontal and parietal activity was associated with increases in both 80 diffusion and drift. Furthermore, diffusion rather than drift explained the most variance in frontal 81 and parietal delay-period activity. In comparison, a subsequent whole-brain regression analysis 82 showed that drift rather than diffusion explained the most variance in delay-period activity in 83 lateral occipital cortex. The results provided a novel interpretation of the functions associated 84 with delay-period activity, suggesting frontoparietal control networks may be engaged to offset load-related diffusive noise while load-related drift is localized to occipital cortex. 85

86

#### 87 **Results**

#### 88 Behavioral performance

Subjects performed a delayed estimation task on line orientations. On different trials, subjects either remembered one orientation (*1O*), or three different orientations (*3O*). For subjects who participated in the fMRI sessions, we first plotted the distribution of their raw responses (n = 16), separately for *1O* and *3O* trials. Recall error, measured as the angular distance between the target orientation and response orientation, increased with increasing memory load, t(15) = 8.27,  $p = 5.68 \times 10^{-7}$ . Furthermore, similar to what has been previously

95	reported for color [14-16], subjects' responses to orientation working memory also clustered
96	around a small number of orientations (Figure 1B).
97	To account for these clusters, we fit the behavioral data with the drift-diffusion model
98	(DDM), which included drift towards attractor locations. For comparison, we also fit the
99	'diffusion-only' model (DOM). Consistent with previous work on color working memory [16],
100	the DDM provided a better fit to behavior than the DOM (difference in cross-validated log-
101	likelihood = 3.67). For the DDM, the diffusion and the drift parameters both increased with
102	memory load ( $t(15) = 4.86$ , $p = 0.0002$ and $t(15) = 2.43$ , $p = 0.028$ , respectively), as did the
103	diffusion parameter from the DOM ( $t(15) = 6.52$ , $p = 9.67 \times 10^{-6}$ ; Figure 1C). When we repeated
104	these analyses on the full set of behavioral data ( $n = 30$ ; including behavior-only subjects), all
105	results were qualitatively similar to those reported above (the average difference in cross-
106	validated log-likelihood across folds was 6.56 between DDM and DOM).
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108	<insert 1="" about="" figure="" here=""></insert>
109	
110	BOLD signal change in IPS and PFC
111	We next examined the BOLD time course in IPS and in PFC during the working memory
112	task, at the two memory loads. We observed the classic pattern of load-sensitive BOLD activity
113	in both ROIs: signal intensity was sustained above baseline across the delay period in both load
114	conditions (all $ps < 0.001$ ), with greater activity for the higher memory load condition (all $ps <$
115	0.01, including the "late-delay" TR, at which BOLD-behavior analyses were carried out; Figure
116	2A and 2B).
117	

118	<insert 2="" about="" figure="" here=""></insert>
119	
120	Modeling load-dependent BOLD activity with behavior at the ROI level
121	To relate load-dependent BOLD activity in parietal and frontal cortex to behavior, we
122	fitted linear regression models with behavioral-model fitted parameters and subject as the
123	independent variables, and BOLD activity as the dependent variable. We first used these
124	regression models to calculate within-subject correlations (ANCOVAs) between behavioral
125	parameters (drift and diffusion) and BOLD activity. The results indicated that BOLD activity in
126	both ROIs correlated significantly with diffusion (IPS diffusion: $r = 0.83$ , $p = 0.00004$ ; PFC
127	diffusion: $r = 0.79$ , $p = 0.0002$ ) and drift (IPS drift: $r = 0.59$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ , $p = 0.012$ ; PFC drift: $r = 0.61$ ; $p = 0.012$ ; PFC drift: $r = 0.61$ ; $p = 0.012$ ; PFC drift: $r = 0.61$ ; $p = 0.012$ ; PFC drift: $r = 0.61$ ; $p = 0.012$ ; $p = 0.$
128	0.009; Figure 2C and 2D).
129	Next, to evaluate the contribution of drift and diffusion, we found the regression model
130	that best explained BOLD activity in the two ROIs. Comparison between the four models of
131	interest indicated that Model 2 (BOLD ~ diffusion (DDM) + subject) explained the most
132	variance in BOLD activity in both IPS and PFC ROIs, and showed the best model performance
133	in terms of AIC and BIC (See Table 1 for a complete list of model comparisons).
134	We also used stepwise regression to examine the relative contribution of drift and
135	diffusion to the prediction of BOLD activity. Starting from Model 3 (BOLD ~ drift (DDM) +
136	diffusion (DDM) + subject), stepwise regression removed drift from the model for both IPS
137	(F(1,14) = 0.35, p = 0.564) and PFC $(F(1,14) = 0.84, p = 0.376)$ , but retained diffusion for both
138	ROIs (diffusion vs. constant model: IPS: $F(32,15) = 4.37$ , $p = 0.003$ ; PFC: $F(32,15) = 4.36$ , $p = 0.003$ ; PFC: $F(32,15) = 4.36$ , $p = 0.003$ ; PFC: $F(32,15) = 4.36$ , $p = 0.003$ ; PFC: $F(32,15) = 4.36$ , $p = 0.003$ ; PFC: $F(32,15) = 4.36$ , $p = 0.003$ ; PFC: $F(32,15) = 4.36$ , $p = 0.003$ ; PFC: $F(32,15) = 4.36$ , $p = 0.003$ ; PFC: $F(32,15) = 4.36$ , $p = 0.003$ ; PFC: $F(32,15) = 4.36$ , $p = 0.003$ ; PFC: $F(32,15) = 4.36$ , $p = 0.003$ ; PFC: $F(32,15) = 4.36$ , $p = 0.003$ ; PFC: $F(32,15) $
139	0.003). Together, these results suggest the level of BOLD activity in both IPS and PFC is most
140	strongly correlated with the amount of diffusive noise in memories.

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142	<insert 1="" about="" here="" table=""></insert>
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144	Modeling load-dependent BOLD activity with behavior at the whole-brain level
145	Lastly, we performed a whole-brain linear regression analysis to explore the relative
146	contribution of drift and diffusion to the BOLD activity of each voxel. Consistent with our ROI-
147	based results, we found significant clusters in bilateral IPS and left frontal cortex with load-
148	dependent BOLD activity that can be better explained by load-dependent changes in diffusion
149	(Figure 3A, red clusters).
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151	<insert 3="" about="" figure="" here=""></insert>
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153	Interestingly, we also observed clusters that showed higher brain-behavior correlation
154	with drift (Figure 3A, green clusters). These clusters were most prominent in in the lateral
155	occipital cortex (LO), in superior postcentral gyrus bilaterally and in right inferior precentral
156	gyrus. Because of the known involvement of occipital cortex in visual working memory, we
157	defined two anatomical ROIs for LO (LO1 and LO2) and repeated with them the ROI-based
158	analyses as previously performed for IPS and PFC.
159	Consistent with previous findings [8, 10-13], BOLD signal intensity in the two LO ROIs
160	returned to baseline during the delay period, with late-delay period activity no different from
161	baseline on <i>1O</i> trials (LO1: $t(15) = 0.300$ , $p = 0.868$ ; LO2: $t(15) = 0.315$ , $p = 0.845$ ) and slightly
162	below-baseline on 3O trials (LO1: $t(15) = 2.754$ , $p = 0.021$ ; LO2: $t(15) = 2.369$ , $p = 0.043$ ;
163	Figure 3B and 3C). ANCOVAs between the behavioral parameters from the DDM and this

BOLD activity revealed trending correlations with drift (LO1: r = -0.48, p = 0.054; LO2: r = -0.44, p = 0.081) and less so with diffusion (LO1: r = -0.44, p = 0.079; LO2: r = -0.34, p = 0.18; Figure 3D and 3E). Furthermore, stepwise regression on Model 3 removed diffusion from the model for both LO1 (F(1,14) = 0.59, p = 0.456) and LO2 (F(1,14) = 0.13, p = 0.727), while drift remained in models for both ROIs (drift vs. constant model: LO1: F(32,15) = 3.98, p = 0.005; LO2: F(32,15) = 4.2, p = 0.004). This result was opposite of what was observed in the IPS and PFC ROIs.

171

## 172 **Discussion**

173 The results of this study provide a new account of the function of load-sensitive activity 174 in IPS and PFC [4, 5]. First, consistent with previous work with color working memory, here we 175 showed that attractor dynamics provided a better account of behavioral data of orientation 176 working memory, compared with classic mixture models that did not take attractor biases into 177 account. Next, and most importantly, the diffusion parameter from the discrete attractor model 178 provided the best account of the load-sensitive delay-period activity of IPS and PFC. In contrast, 179 in LO where aggregate levels of late delay-period activity were at or below baseline levels, load-180 sensitive fluctuation in this activity was better explained by drift. Thus, our results provide the 181 first evidence to our knowledge that load-related imprecision in working memory, known to 182 entail increases in random diffusion and in drift towards stable attractor state, engages control-183 related circuits of IPS and PFC and sensory-related circuits of LO, respectively. 184 By definition, working memory is guided by information specific to the current trial.

185 Nevertheless, working memory is also often influenced by many other factors, such as sensory
186 history [17] and prior knowledge. In working memory for color, the influence of prior

187 knowledge is reflected as clustered responses around a small number of specific color values, 188 even when the distribution of sample colors is uniform [14-16]. The present results show that this 189 phenomenon generalizes to another low-level visual feature, orientation, and these biases 190 increased with increasing memory load. Together with those of Panichello et al. (2019), our 191 results indicate that dynamical systems offer a useful framework within which to understand the 192 influence of trial-nonspecific factors on working memory performance.

193 Neurally, delay-period neural activity in IPS and PFC increased with increasing memory 194 load, and we showed that this load-dependent change in BOLD activity was mainly related to 195 load-dependent changes in diffusion rather than drift. Therefore, load-related activity change in 196 IPS and PFC is likely related to random diffusion processes, rather than systematic biases 197 towards attractors. The random noise could be related to noise in representations when memories 198 are held in IPS/PFC or related to greater engagement of control processes when working memory 199 has greater diffusion. For example, a recent study has found that delay-period activity in IPS is 200 more sensitive to the demands of context binding than of memory load per se. By this account, 201 increases in diffusion were likely due, at least in part, to increased interference between 202 representations of stimulus content and stimulus context, which would be expected to place 203 greater demands on a frontoparietal priority map controlling visually guided behavior [8]. In 204 comparison, load-related activity in LO was more sensitive to load-related changes in drift to 205 particular stimulus values, rather than diffusion. This result is consistent with the idea that prior 206 knowledge shapes feature tuning in visual cortex, resulting in biased tuning responses to 207 different visual features at early stages of cortical processing [18].

When considering these findings, it is important to not think of these factors as working in isolation. In frontoparietal cortex, for example, estimating drift is still necessary, as it allows

for a more accurate model of diffusion, that can better predict neural signals in these regions. Moreover, it is important to note that in terms of parameter fitting, the drift parameter relies inferring the shape of attractor landscape across the entire stimulus space, and therefore both the number of trials and the uniformity of target distribution can have a significant impact on the fitted outcome. It is possible that future studies acquiring more trials, and/or applying more uniformly distributed targets, will lead to improved model fit of drift, and increases in the variance explained by this parameter.

217 In previous studies emphasizing stimulus-specific representations of visual working 218 memory, we have argued that disparate patterns of results in frontoparietal versus occipital 219 cortex are consistent with a functional distinction between these two regions, with the former 220 more strongly associated with control and the latter with stimulus representation [8, 10]. Here, 221 we see that stimulus-nonspecific factors, as reflected in the relationship between load-dependent 222 changes in behavior (drift and diffusion) and delay-period activity, are also consistent with this 223 distinction. Taken together, the results from higher-order frontal and parietal cortex and low-224 level occipital cortex suggest that imprecision in working memory can be caused by a 225 combination of effects of noise in parietal and frontal cortex, and of stimulus-related biases in 226 occipital cortex.

227

#### 228 Method

229 Subjects

The results reported here are from analyses carried out on existing data collected for other purposes [19, 20]. Thirty individuals (10 males, mean age  $20.7 \pm 2.3$  years) participated in the behavioral session of the study, and sixteen of these (8 males, mean age  $20.6 \pm 1.8$  years) also

participated in two subsequent fMRI scanning sessions. All were recruited from the University of
Wisconsin–Madison community. All had normal or corrected-to-normal vision, reported no
neurological or psychiatric disease, and provided written informed consent approved by the
University of Wisconsin–Madison Health Sciences Institutional Review Board. Anatomical
scans from the fMRI session were also screened by a neuroradiologist, and no abnormalities
were detected. All subjects were monetarily compensated for their participation.

239

## 240 Stimuli and procedure

241 All stimuli were created and presented using Matlab (MathWorks, Natick, MA) and 242 Psychtoolbox 3 extensions [21, 22]. In the behavioral session, stimuli were presented at a 243 viewing distance of 62 cm on an iMac screen, with a refresh rate of 60 Hz. Subjects registered 244 behavioral responses on a trackball response pad. In the fMRI session, stimuli were projected 245 onto a 60-Hz Avotec Silent Vision 6011 projector (Avotec, Stuart, FL), and viewed through a 246 coil-mounted mirror in the MRI scanner at a viewing distance of 69 cm. Subjects registered 247 behavioral responses on a MR-compatible trackball response pad (Current Designs Inc., 248 Philadelphia, PA).

There were three types of stimuli: oriented bars, color patches, or luminance patches. Each oriented-bar stimulus appeared as a black line (width =  $0.08^{\circ}$ ) bisecting a white circle (radius =  $2^{\circ}$ ). Line orientations were drawn from a pool of 9 orientations ranging from 0 to  $160^{\circ}$ , in  $20^{\circ}$  increments, with a random jitter of  $1-5^{\circ}$  added to each stimulus. Color patches were circular patches (radius =  $2^{\circ}$ ) filled with one color drawn from a pool of 9 colors that were equidistant in CIEL\*a\*b color space (L = 70, a = 20, b = 38, radius =  $60^{\circ}$ ), with a random jitter of  $1-5^{\circ}$ . Luminance patches were rendered as a gray circular patch (radius =  $0.83^{\circ}$ ) inside a white

annulus (radius =  $2^{\circ}$ ), and the luminance of the patches were drawn from 9 grayscale values from [0.03, 0.03, 0.03] to [0.97, 0.97, 0.97], in steps of 0.1175. Throughout the experiment, the background screen color was gray [0.5, 0.5, 0.5].

259 There were three different trial types. On "10" trials, one oriented bar was presented at 260 one of four possible locations (45°, 135°, 225°, 315° relative to central fixation, with an eccentricity of 5°) for 4 s. Stimulus offset was followed by a mask (white circle [radius =  $2^{\circ}$ ] 261 262 bisected by 18 black bars [width =  $0.08^{\circ}$ ] intersecting at their midpoints and each differing in 263 orientation from its neighbors by  $10^\circ$ ; 0.25 s) and a delay period (7.75 s) during which subjects 264 maintained central fixation. Recall was prompted by the onset of a stimulus circle appearing at 265 the same location as the sample, a response wheel centered on fixation (inner radius =  $7.2^{\circ}$ , outer 266 radius of 9.2°), and a cursor (a conventional "mouse" arrow) located at central fixation. Twenty 267 oriented lines (radius =  $1.8^\circ$ , width =  $0.05^\circ$ , ranging in orientation from  $0^\circ$  to  $171^\circ$  in steps of  $9^\circ$ ) 268 were displayed with equal spacing along the response wheel, and subjects registered their 269 memory of the sample orientation by moving the cursor to the appropriate location on the 270 response wheel and registering that location with a button press. At the onset of the recall 271 display, the stimulus patch was rendered with a randomly determined value rendered in the 272 format of the sample stimuli, and as soon as the subject began to move the cursor (with the 273 trackball) the stimulus patch took on the value corresponding to the location on the response 274 wheel that was nearest to the cursor. Responses were required within 4 s, while the circle and 275 wheel remained on the screen. The angle of rotation of the response wheel was randomized 276 across trials, to prevent subjects from preparing their response during the delay period. 277 "30" trials were similar to "10" trials, except three oriented bars, each with a different

278 orientation, were displayed in three of the four possible sample locations, and, at time 12 s, the

sample to be recalled was indicated by the location of the stimulus circle in the recall array. For
each *3O* trial, sample values were selected randomly, without replacement, from the pool of 9
possible orientations (Figure 1A).

On "*101C1L*" trials, 1 oriented bar, 1 color patch, and 1 luminance patch were presented, and during the response stage subjects were tested, unpredictably, on their memory for one of these stimuli. The response wheel for color and luminance was the same size as the orientation wheel, but displayed 180 possible color or luminance values.

286 The behavioral session contained two blocks of *1O* and *3O* trials, and three blocks of

287 *101C1L* trials. Each block contained 50 trials, and block order was counterbalanced across

subjects. The 10 and 30 blocks contained 25 trials each for 10 and 30, and the 101C1L blocks

contained 17 probes of two of the three categories, and 16 of the remaining one. The selection of

290 the categories was randomized across blocks, yielding 50 trials for each category across three

blocks.

There were two fMRI scanning sessions. The first scanning session included four 18-trial blocks of 9 *30* trials and 9 *101C1L* trials (with 3 probes each for orientation, color, and luminance), yielding a total of 36 trials for each of these load-of-3 trial types. These four blocks were followed by eight 18-trial blocks of *10* trials. The second session included twelve blocks of *10* trials. To match the number of trials between conditions in fMRI data, two of the twenty *10* blocks were randomly selected for each subject for further analyses.

We introduce the *101C1L* condition here only for the completeness of experimental design. All subsequent analyses focused on *10* and *30* trials for load-related changes in behavioral and neural data.

301

# 302 Behavioral modeling

303	We fitted data from the behavioral session using a discrete attractor model [16]. This
304	circular drift-diffusion model (DDM) fits the dynamic evolution of memories with two distinct
305	processes: random noise (diffusion); and systematic drift towards one of several stable attractors.
306	Notably, when the drift parameter is removed, the remaining diffusion-only model (DOM) is
307	equivalent to a classic mixture model [23]. Both parameters are rates, with a unit of rad/s
308	indicating the rate of diffusion and the maximum instantaneous drift rate. Unlike the Panichello
309	et al. (2019) study, here we fitted behavioral data without separating out encoding and delay
310	processes, because the length of memory delays was not manipulated in this experiment. The
311	comparison between performance of the DDM and DOM models was evaluated by computing a
312	10-fold cross-validated log-likelihood value.
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314	fMRI Data acquisition
	<i>fMRI Data acquisition</i> Whole-brain images were acquired with a 3 Tesla GE MR scanner (Discovery MR750;
314	
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<ul><li>314</li><li>315</li><li>316</li></ul>	Whole-brain images were acquired with a 3 Tesla GE MR scanner (Discovery MR750; GE Healthcare, Chicago, IL) at the Lane Neuroimaging Laboratory at the University of
<ul><li>314</li><li>315</li><li>316</li><li>317</li></ul>	Whole-brain images were acquired with a 3 Tesla GE MR scanner (Discovery MR750; GE Healthcare, Chicago, IL) at the Lane Neuroimaging Laboratory at the University of Wisconsin–Madison HealthEmotions Research Institute (Department of Psychiatry). Functional
<ul> <li>314</li> <li>315</li> <li>316</li> <li>317</li> <li>318</li> </ul>	Whole-brain images were acquired with a 3 Tesla GE MR scanner (Discovery MR750; GE Healthcare, Chicago, IL) at the Lane Neuroimaging Laboratory at the University of Wisconsin–Madison HealthEmotions Research Institute (Department of Psychiatry). Functional images were acquired with a gradient-echo echo-planar sequence (2 sec repetition time (TR), 25
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<ul> <li>314</li> <li>315</li> <li>316</li> <li>317</li> <li>318</li> <li>319</li> <li>320</li> </ul>	Whole-brain images were acquired with a 3 Tesla GE MR scanner (Discovery MR750; GE Healthcare, Chicago, IL) at the Lane Neuroimaging Laboratory at the University of Wisconsin–Madison HealthEmotions Research Institute (Department of Psychiatry). Functional images were acquired with a gradient-echo echo-planar sequence (2 sec repetition time (TR), 25 msec echo time (TE), 60° flip angle) within a $64 \times 64$ matrix (40 sagittal slices, 3.5mm isotropic). Each of the fMRI scans generated 215 volumes. A high-resolution T1 image was also
<ul> <li>314</li> <li>315</li> <li>316</li> <li>317</li> <li>318</li> <li>319</li> <li>320</li> <li>321</li> </ul>	Whole-brain images were acquired with a 3 Tesla GE MR scanner (Discovery MR750; GE Healthcare, Chicago, IL) at the Lane Neuroimaging Laboratory at the University of Wisconsin–Madison HealthEmotions Research Institute (Department of Psychiatry). Functional images were acquired with a gradient-echo echo-planar sequence (2 sec repetition time (TR), 25 msec echo time (TE), 60° flip angle) within a 64 × 64 matrix (40 sagittal slices, 3.5mm isotropic). Each of the fMRI scans generated 215 volumes. A high-resolution T1 image was also acquired for each session with a fast spoiled gradient-recalled-echo sequence (8.2 msec TR, 3.2

324 fMRI Data preprocessing

325	Functional MRI data were preprocessed using AFNI (http://afni.nimh.nih.gov) [24]. The
326	data were first registered to the first volume of the first run, and then to the T1 volume of the first
327	scan session. Six nuisance regressors were included in GLMs to account for head motion
328	artifacts in six different directions. The data were then motion corrected, detrended (linear,
329	quadratic, cubic), converted to percent signal change, and spatially smoothed with a 4-mm
330	FWHM Gaussian kernel. For the whole-brain analysis, the data were further aligned to the MNI-
331	ICBM 152 space [25].
332	

333 Region of interest (ROI) definition

334 We first defined anatomical ROIs using existing anatomical atlases, and warped them 335 back to each subject's structural scan in native space. Parietal anatomical ROIs were created by 336 extracting intraparietal sulcus (IPS) masks IPS0-5 from the probabilistic atlas of Wang and 337 colleagues [26], merging them, and collapsing over the right and left hemispheres. Lateral 338 prefrontal cortex (PFC) anatomical ROIs were created by extracting masks of the superior, 339 middle, and inferior frontal gyri supplied by AFNI, merging them, and collapsing over the right 340 and left hemispheres. Lateral occipital anatomical ROIs were created by extracting masks for 341 LO1 and LO2, from the probabilistic atlas of Wang and colleagues [26], merging them, and 342 collapsing over the right and left hemispheres.

To find the functionally activated voxels within the anatomical atlases, a conventional mass-univariate general linear model (GLM) analysis was implemented in AFNI, with sample, delay and probe periods of the task modeled with boxcars (4 sec, 8 sec, and 4 sec in length, respectively) that were convolved with a canonical hemodynamic response function. Across the whole brain, we identified the 2000 voxels displaying the strongest loading on the contrast [delay

348 - baseline], collapsing over all three conditions. The intersection of these 2000 voxels and the two anatomical masks defined the two functional ROIs in subsequent analyses: the IPS ROI and 349 350 the PFC ROI. On average, the IPS functional ROI contained  $463 \pm 177$  voxels, the PFC 351 functional ROI contained  $314 \pm 86$  voxels; the two anatomical LO ROIs contained  $404 \pm 57$  and 352  $456 \pm 69$  voxels, respectively. 353 354 *Univariate analyses* 355 We calculated the percent signal change in BOLD activity relative to baseline for each 356 time point during the working memory task; baseline was chosen as the average BOLD activity 357 of the first TR of each trial. The BOLD signal change was averaged across trials within each 358 condition, and across all voxels within each ROI. Statistical significance of BOLD activity 359 against baseline was assessed using two-tailed, one-sample t-tests against 0, and the obtained p 360 values were corrected across loads and time points using FDR (False Discovery Rate) [27]. 361 Statistical difference of BOLD activity between 10 and 30 at each time point was assessed 362 using two-tailed paired t-tests, and similarly the obtained p values were FDR corrected across 363 time points. 364

365 Brain-behavior correlation and model comparisons

Following previous work [8-10], we used an analysis of covariance (ANCOVA) method to evaluate the correlated sensitivity to trial type (i.e., *10* vs. *30*) across pairs of task-related variables (i.e., BOLD activity vs. behavioral parameter). Unlike simple correlations, ANCOVA accommodates the fact that each subject contributes a value for each level of trial type. It

- 370 removes between-subject differences and assesses evidence for "within-subject correlation"
- between the two task-related variables [28].
- 372 Mathematically, within-subject correlations were implemented as linear regression
- 373 models, and were calculated for *drift* and *diffusion* separately, where *subject* is a dummy variable
- for trial types (10 and 30) of each subject, and BOLD is BOLD signal from time 12 s ("late
- 375 delay-period" activity):
- 376 Model 1: BOLD ~ drift (DDM) + subject;
- 377 Model 2: BOLD ~ diffusion (DDM) + subject;
- 378 The within-subject correlation r for drift or diffusion was calculated as:

379 
$$r = \frac{\sqrt{SS_{drift or diffusion}}}{\sqrt{SS_{drift or diffusion} + SS_{error}}}$$

380 where SS stands for sum of squares.

381 To compare between the performance of different regression models, we included two

382 more models, one full model that took both drift and diffusion into account, and one control

383 model that used diffusion from the DOM model:

384 Model 3: BOLD ~ drift (DDM) + diffusion (DDM) + subject;

385 Model 4: BOLD ~ diffusion (DOM) + subject.

386 Model performance was evaluated by comparing Akaike Information Criterion (AIC),

387 Bayesian Information Criterion (BIC), and adjusted  $R^2$  (explained variance of the model after

- adjusting for the number of predictors) of each model.
- 389 Lastly, we performed stepwise regression to evaluate the contribution of the drift and
- 390 diffusion parameters to the prediction of BOLD activity. The regression model started with
- 391 Model 3, after the initial fit, the predictors in the model were examined one by one, and the
- 392 predictor with a p > 0.10 in the *F* test after removal was removed.

393

## 394 Whole-brain regression analysis

395 To explore brain areas that showed activity sensitive to either the drift or diffusion 396 parameter, we used a whole-brain exploratory analysis to find voxels with activity that can be 397 best explained by either drift or diffusion. To this end, all subjects' data were first normalized to 398 the MNI-ICBM 152 space [25], and for each voxel we fit Models 1 and 2 to the BOLD activity 399 of that voxel. The model with a higher adjusted  $R^2$  for each voxel was selected as the best fitting 400 for that voxel, and we used the *p*-value of the selected model (*F*-test on regression vs. constant 401 model) for statistical significance. To correct for multiple comparisons, we applied the False 402 Discovery Rate (FDR) method to the *p*-values of the selected model across voxels. To avoid 403 overinterpretation, we also applied a threshold in model selection using BIC [29], such that only 404 voxels with a significant *p*-value after correction, and in which the drift or diffusion model 405 outperformed the other by a BIC  $\geq 2$ , remained in the final report. Therefore, we identified 406 voxels with load-dependent BOLD activity that could be better explained by load-dependent 407 changes in drift, or in diffusion, at the whole-brain level. Results from the whole-brain analysis 408 were displayed on the cortical surface reconstructed with FreeSurfer 409 (http://surfer.nmr.mgh.harvard.edu; [30, 31]) and visualized with SUMA in AFNI 410 (http://afni.nimh.nih.gov) [24].

412	Figure Legends
413	Figure 1A. Trial sequence of the fMRI task and Behavioral performance
414	A. For the data analyzed in the current study, participants remembered either one orientation
415	(10), or three orientations (30). Sample stimuli were presented on the screen for 4 s, followed
416	by a brief mask period of 0.25 s. After a delay of 7.75 s, participants rotated the needle of the
417	response wheel to indicate the remembered orientation at the probed location.
418	<b>B</b> . The raw response distribution of <i>1O</i> and <i>3O</i> trials, indicated by the gray histograms. The
419	black lines indicate the envelope of target distribution, and pink and green lines indicate the
420	envelope of response distribution, for 10 and 30 trials separately.
421	C. Model-free and model-based behavioral performance. From left to right panel shows mean
422	error, diffusion from the DOM model, drift from the DDM model, and diffusion from the DDM
423	model. Error bars indicate $\pm 1$ SEM.
424	
425	Figure 2. BOLD activity and brain-behavior correlations in IPS and PFC
426	A. Trial-averaged BOLD activity in the IPS functional ROI. B. Time course of BOLD activity in
427	the PFC functional ROI. Pink and green lines correspond to the 10 and 30 conditions,
428	respectively. Error bars indicate $\pm$ 1 SEM. C. Within-subject correlations between behavioral
429	parameter from DDM (drift and diffusion plotted separately) and IPS BOLD activity, at "late
430	delay" time point (12 s). D. within-subject correlations between behavioral parameter (drift or
431	diffusion) and PFC BOLD activity. In each plot, data from each subject are plotted in a different
432	color, and the "1" and "3" symbols correspond to values from 10 and 30 trials, respectively.
433	Lines illustrate the best fit of the group-level linear trend (i.e., the within-subject correlation) in
434	relation to individual subject data.

435

# Figure 3. Whole-brain regression analysis with drift and diffusion and ROI-based results in LO

- 438 A. Whole-brain regression with drift and diffusion. Green denotes voxels showing load-
- 439 dependent BOLD activity that can be better explained by load-dependent changes in drift, and
- 440 Red denotes voxels showing load-dependent BOLD activity that can be better explained by load-
- 441 dependent changes in diffusion. For visualization purposes, results were clusterized at a

threshold of 20 voxels. The left two panels show results from the left hemisphere, and the right

- 443 two panels show results from the right hemisphere. The significance of the regression models
- 444 was corrected using the FDR method at p < 0.05.
- 445 B. Trial-averaged BOLD activity in the LO1 anatomical ROI. C. Time course of BOLD activity
- 446 in the LO2 anatomical ROI. Pink and green lines correspond to the *1O* and *3O* conditions,
- 447 respectively. Error bars indicate  $\pm 1$  SEM. **D**. Within-subject correlations between behavioral
- 448 parameter from DDM (drift and diffusion plotted separately) and LO1 BOLD activity, at "late
- 449 delay" time point (12 s). E. within-subject correlations between behavioral parameter (drift or
- 450 diffusion) and LO2 BOLD activity. In each plot, data from each subject are plotted in a different
- 451 color, and the "1" and "3" symbols correspond to values from *1O* and *3O* trials, respectively.
- 452 Lines illustrate the best fit of the group-level linear trend (i.e., the within-subject correlation) in
- 453 relation to individual subject data.

454

## 455 **Table 1**: Comparison between different regression models

Model	adjusted R <sup>2</sup>	AIC	BIC
IPS			

Model 1	0.237	29.3792	54.2967
Model 2	0.635	5.7543	30.6718
Model 3	0.619	6.9660	33.3493
Model 4	0.580	10.2552	35.1757
PFC			
Model 1	0.412	14.1163	39.0338
Model 2	0.659	-3.2714	21.6461
Model 3	0.652	-2.8174	23.5658
Model 4	0.566	4.3899	29.3075

456

457

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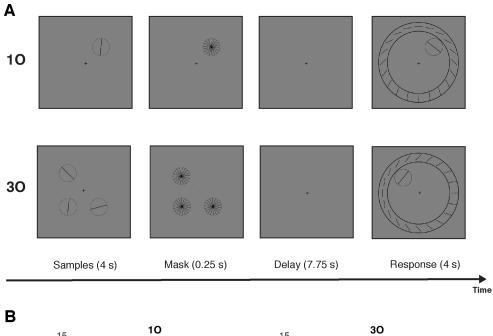
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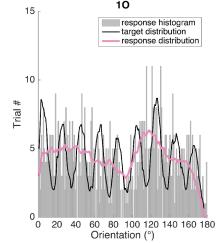
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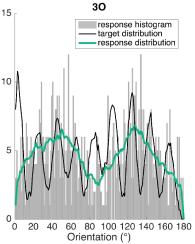
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580 Figure 1



Trial #



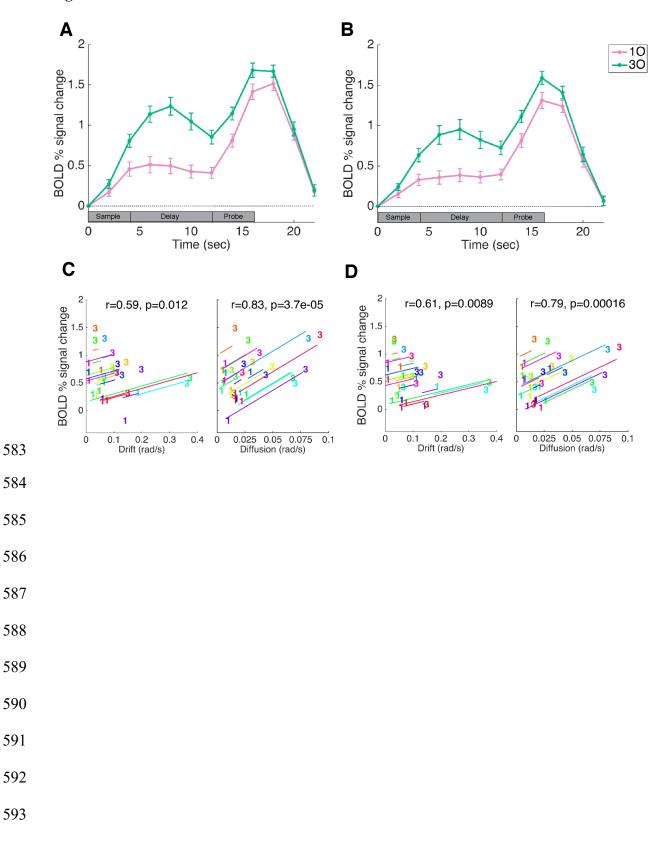


Drift-DDM Diffusion-DDM Mean error Diffusion-DOM 0.5 0.06 0.25 0.06 0.05 0.05 0.4 0.2 0.04 0.04 0.3 0.15 rad/s s/0.03 rad s/pg 0.03 0.2 0.1 0.02 0.02 0.1 0.05 0.01 0.01 0 0 0 0 30 30 30 10 10 10 10 30

581

С

582 Figure 2



# 594 Figure 3

