1 **Histo-molecular differentiation of renal cancer subtypes by mass**

2 **spectrometry imaging and rapid proteome profiling of formalin-fixed**

3 **paraffin-embedded tumor tissue sections**

Uwe Möginger[1,§], Niels Marcussen[2], Ole N. Jensen[1*]

[1]Department of Biochemistry & Molecular Biology and VILLUM Center for Bioanalytical

Sciences, University of Southern Denmark, DK-5230 Odense M, Denmark.

[2]Institute for Pathology, Odense University Hospital, DK-5000 Odense C, Denmark.

Corresponding author:

Professor Ole N. Jensen, PhD, email: jenseno@bmb.sdu.dk

Department of Biochemistry & Molecular Biology and VILLUM Center for Bioanalytical

Sciences, University of Southern Denmark, DK-5230 Odense M, Denmark.

[§]Present address: Global Research Technologies, Novo Nordisk A/S, Novo Nordisk Park, DK-
2760 Måløv, Denmark

Keywords:

Renal Cell Cancer, MALDI Mass Spectrometry Imaging (MALDI MSI), Microproteomics,

Statistical Classification, Liquid Chromatography Mass Spectrometry (LC-MS)

Abstract

Pathology differentiation of renal cancer types is challenging due to tissue similarities or overlapping histological features of various tumor (sub)types. As assessment is often manually conducted outcomes can be prone to human error and therefore require high-level expertise and experience. Mass spectrometry can provide detailed histo-molecular information on tissue and is becoming increasingly popular in clinical settings. Spatially resolving technologies such as mass spectrometry imaging and quantitative microproteomics profiling in combination with machine learning approaches provide promising tools for automated tumor classification of clinical tissue sections.

In this proof of concept study we used MALDI-MS imaging (MSI) and rapid LC-MS/MS-based microproteomics technologies (15 min/sample) to analyze formalin-fixed paraffin embedded (FFPE) tissue sections and classify renal oncocytoma (RO, n=11), clear cell renal cell carcinoma (ccRCC, n=12) and chromophobe renal cell carcinoma (ChRCC, n=5). Both methods were able to distinguish ccRCC, RO and ChRCC in cross-validation experiments. MSI correctly classified 87% of the patients whereas the rapid LC-MS/MS-based microproteomics approach correctly classified 100% of the patients.

This strategy involving MSI and rapid proteome profiling by LC-MS/MS reveals molecular features of tumor sections and enables cancer subtype classification. Mass spectrometry provides a promising complementary approach to current pathological technologies for precise digitized diagnosis of diseases.

Introduction

Kidney cancer (renal cell carcinoma, RCC) accounts for 2.2% of all diagnosed cancers and is the 13th most common cause of cancer deaths worldwide [1]. Clear cell renal cell carcinoma (ccRCC) constitutes 70% of all kidney cancers [2] and exhibits the highest rate of metastasis among renal carcinomas. Two other common but less aggressive subtypes of renal carcinoma are chromophobe renal cell carcinoma (ChRCC) and the essentially benign renal oncocytoma (RO), which account for 5% and 3-7 % of all cases, respectively [3,4]. The ability to distinguish between the malignant cancer types ccRCC and ChRCC and the benign RO is crucial for a patient in terms of prognosis, progression and intervention strategies as severe as total nephrectomy. Histopathological kidney cancer diagnostics faces many challenges in daily routine. Typically, test panels consisting of a combination of different chemical and immuno-histochemical staining methods are used to systematically obtain a diagnosis [5]. Overlapping histological features can make it difficult to differentiate tumor types. Analysis, interpretation and diagnosis/prognosis greatly rely on visual inspection and the experience of the involved clinical pathologists. Complementary techniques such as MRI and electron microscopy involve costly instrumentation. Moreover, specific antibodies for staining can be expensive or unavailable for certain molecular targets. Mass spectrometry is emerging as a promising new tool in translational research, from molecular imaging of tissue sections to deep protein profiling of tissue samples [6]. The digital data readout provided by high mass accuracy mass spectrometry and feasibility of molecular quantification makes it a very attractive technology in translational research for investigating human diseases and for diagnostics and prognostics purposes in the clinic. Improvements in mass spectrometry

instrument performance and computational analysis paved the way for applications in clinical

microbiology [7] and clinical genetics analysis [8]. The fact that mass spectrometry can be

applied to a variety of different bio-molecules such as peptides, lipids, nucleic acid makes it

extremely versatile and expands the translational and diagnostic possibilities greatly [8-11].

Molecular imaging of tissue sections by MALDI mass spectrometry (MSI) was introduced

more than 20 years ago [12,13] and it has been applied in translational research and clinical

applications, to study injuries, diseases, or distinguish between different cancer types such as

Pancreatic Ductal Adenocarcinoma or Epithelial Ovarian Cancer Histotypes [14-18].

Mass spectrometry-based proteomics relies on advanced LC-ESI-MS/MS technology, where

peptide mixtures are separated by liquid chromatography (LC) prior analysis by electrospray

ionization tandem mass spectrometry (ESI MS/MS) and protein identification by protein

database searching [19,20]. Current LC-MS/MS strategies enable comprehensive quantitative

protein profiling from tissues and body fluids [21,22]. While having been used to identify potential

biomarkers or new candidate cancer targets and molecular signaling networks the relatively

long LC gradients (hours) and extensive sample preparation protocols make it difficult to

apply in a routine clinical setting. Modern mass spectrometers are steadily increasing in

sensitivity and scanning speed [23]. In addition, improved chromatographic systems that enable

rapid solid phase extraction integrated with reproducible separations are emerging [24-27],

enabling fast (minutes) and sensitive (nanogram) analysis of complex biological samples.

We hypothesized that histo-molecular information from both MALDI MS imaging (MSI), *in situ*

protein digestion and LC-MS/MS applied to detailed characterization of 5 μm cancer FFPE

tissue sections will provide spatial molecular maps and sufficiently deep proteome profiles to

characterize and classify tumor subtypes. We investigated this by testing a series of

malignant and benign renal carcinomas, including clear cell renal cell carcinoma (ccRCC),

chromophobe renal cell carcinoma (ChRCC) and renal oncocytoma (RO). We obtained histo-

molecular images at a resolution of 150µm x 150µm that sufficed to spatially resolve features

to distinguish tumor subtype areas from surrounding tissue. Miniaturized sample preparation

by *in situ* protein digestion was used to recover peptides from distinct areas of the FFPE

tumor sections for rapid proteome profiling by LC-MS/MS.

94　Material and Methods:

95　Materials

Xylene (analytical grade), ammonium bicarbonate, Sodium citrate, trifluor-acetic acid (TFA),

formic acid (FA), acetic acid (AcOH), acetonitrile (ACN), methanol and α-Cyano-4-

hydroxycinnamic acid (CHCA) were purchased from Sigma (). Polyimide coated fused silica

capillary (75 µm ID) was from PostNova, C_{18} Reprosil Pur reversed phase material was from

Dr. Maisch (Ammerbuch-Entringe, Germany), recombinant Trypsin was purchased from

Promega (WI. USA), Indium-tin-oxide (ITO) glass slides were purchased from Bruker

(Bremen, Germany), water was Milli-Q filtered.

103　Formalin fixed paraffin embedded samples:

Patient samples were collected at Odense University Hospital, Denmark. All samples were obtained upon patient's consent. Formalin fixed paraffin embedded (FFPE) tissues from 11 RO patients, 12 ccRCC patients and 5 ChRCC patients were used for LC-MSMS analysis (for ChRCC due to the lower number of patients 2 subsequent slides were used from 2 patients adding up to a total of 7 sections). Out of the patient cohort 9 RO, 9 ccRCC and 5 ChRCC were used for mass spectrometry imaging analysis.

Tissue preparation:

Preparation of formalin fixed paraffin embedded samples

FFPE blocks were cut into 5 μm thick sections and mounted onto indium tin oxide (ITO) covered glass slides (for MSI) or regular microscopy glass slides (for LC-MS/MS). Before deparaffination slides were left on a heated block at 65° C for 1 hour to improve adhesion (an overview on the used FFPE samples can be found in supplementary table S1 and S2).

Deparaffination

FFPE section slides were incubated in Xylene for an initial 10 min. and then another 5 min. using fresh solution each time. Slides were shortly dipped into 96% EtOH before they were washed for 2 min in a mixture of chloroform/Ethanol/AcOH (3:6:1; v:v:v). The slides were then washed in 96% EtOH, 70% EtOH, 50% EtOH and Water for 30 sec. each.

Antigen retrieval

Tissue slides were heated in 10mM citric acid buffer pH 6 for 10 min in a microwave oven at 400 Watt (just below the boiling point) before left for further 60 min incubation at 98°C on a

heating plate. Slides were cooled down to room temperature and incubated for 5 minutes in

25 mM ammonium bicarbonate (ABC) buffer. Slides were allowed to dry before application of

trypsin protease.

Tryptic digest

For MALDI MS imaging:

20µg of Trypsin (Promega) was used per slide and was dissolved at a concentration of

100ng/µl in 25mM ABC /10% ACN before being deposited on the tissue using the

iMatrixSpray [28] device equipped with a heating bed (Tardo Gmbh, Subingen, Switzerland)

using the following settings: sprayer height = 70mm, speed = 70mm/s, density = $1\mu L/cm^2$,

line distance= 1 mm , gas pressure= 2.5 bar, heat bed temperature= 25°C . After trypsin

deposition the slides were incubated in a humid chamber containing 10mM ABC/ 50% MeOH

at 37°C over night.

For *on-tissue* digest intended for LC-MS/MS proteome profiling:

Droplets of 2µl Trypsin solution (50ng/µL in 25mM ABC /10%ACN, 0.02%SDS) were

deposited using a gel loading pipet tip. Droplets were placed on 3-4 different tumor areas of

each FFPE tissue section. The droplets were shortly allowed to dry in order to prevent

spreading across the tissue. Slides were transferred to a humid chamber (10mM ABC /50%

MeOH) for overnight digestion at 37°C. After digest the digestion spots were extracted twice

with 2µL of 0.1% FA and twice with 1.5µL of 30%ACN. Samples were collected, speedvac

dried. Before injection samples were reconstituted in 0.05%TFA and shortly spun down.

Matrix application

Matrix solutions were freshly prepared from recrystallized α-cyano-4-hydroxycinnamic acid (CHCA) matrix (10mg/mL in 50% Acetonitrile 1% TFA). Matrix was sprayed using the iMatrixSpray (Tardo, Switzerland). Temperature of the heatbed was set at 25°C. The sprayer distance was set to 70mm. Spray speed was set to 100 mm/s. Matrix was sprayed in 3 rounds: 8 cycles with a flowrate of 0.5µl/cm^2 line distance of 1mm, 8 cycles of 1µl/cm^2 line distance of 1mm, 8 cycles of 1µl/cm^2 and a line distance of 2mm.

MALDI MS Imaging data acquisition

Optical images of the tissue were obtained before matrix application using a flatbed scanner (Epson) at resolutions of 2400dpi. The imaging data was acquired via FlexImaging software (Bruker, Daltonics, Bremen, version 3.1) with 500 shots/ pixel on a Ultraflextreme MALDI-TOF/TOF MS (Bruker Daltonics, Bremen) equipped with a SmartBeam laser (Nd:YAG 355 nm). External mass calibration was performed with a tryptic digest of bovine serum albumin (Sigma). Spatial resolution was set to 150µm in x- and y-direction. Mass spectra were acquired in positive ion reflector mode in the range *m/z* 600-3500.

LC-MS/MS analysis

LC-MS/MS data was acquired by an Orbitrap Q-Exactive HF-X (Thermo, Bremen) coupled to an Ultimate 3000 capillary flow LC-system. Setup was adopted and modified from Thermo Scientific Technical note: 72827. Peptide samples were loaded at 150µl/min (2% ACN, 0.05% TFA) for 30 sec onto a 5µm, 0.3 x 5 mm, Acclaim PepMap trapping cartridge (Thermo

Scientific). Samples were then eluted onto a pulled emitter analytical column (75µm ID,

15cm). The analytical column was "flash-packed" [29] with C_{18} Reprosil Pur resin (3µm) and

connected by Nanoviper fittings and a reducing metal union (Valco, Houston, TX). The

flowrate of the 15 min gradient was 1.2 µL/min with solvent A: 0.1% formic acid (FA) and

solvent B: 0.1% FA in 80% ACN. Gradient conditions for solvent B were as followed: 8% to

25% in 10 min, 25% to 45% in 1.7 min. The trapping cartridge and the analytical column were

washed for 1 min at 99%B before returning to initial conditions. The column was equilibrated

for 2 min.

Data Processing of MALDI MS imaging data

The data was baseline subtracted, TIC normalized and statistically recalibrated and then

exported into imzML format [30] using the export function of FlexImaging software (Bruker). The

exported mass range was 600-3000 m/z with a binning size of 9600 data points. The imzML

files were imported into the R environment (version: 3.4.1) and further processed and

analyzed using the R MSI package: Cardinal (version: 2.0.3 & 2.4) [31]. In order to extract pixels

of tumor tissue each sample was preprocessed as follows: peaklist was generated by peak

picking in every 10th spectrum and subsequent peak alignment. The whole data was then

resampled using the "height" option and the previous created peaklist as spectrum reference.

PCA scores were plotted using car-package (version 3.0.6). Samples were clustered using

spatial shrunken centroid clustering [32]. Subsequently, pixel coordinates of cluster containing

tumor areas (HE-stain comparison, supplementary material 1: Figure S3) were extracted and

if necessary manually trimmed, so that result files predominantly contained data from tumor

areas. The obtained coordinates were then used to extract the corresponding pixel from the

unprocessed imzML file. Each tumor type was assigned with a diagnosis factor (ccRCC, RO

or ChRCC), which was later used as y-argument in the cross-validation. All extracted imaging

acquisition files were further restricted to a mass range of m/z 700-2500. Data was resampled

with step size 0.25 Da to allow combining them into one file for further processing.

Classification and cross validation were performed using partial least square discriminant

analysis (PLS-DA) [33]. PLS components were tested for optimum with 34 components

(supplementary material 1: Figure S1).

LC-MS/MS data processing

The MaxQuant [34] software package (version 1.5.7.0) was used for protein identification and

label-free protein quantitation. LC-MS/MS data was searched against the Swissprot human

proteome database, using standard settings and "match between runs" enabled.

Data filtering, processing and statistical analysis of the MaxQuant output files was performed

using the Perseus [35] framework (version 1.6.1.3). Data was filtered excluding the following

hits: only identified by site, contaminants and reversed. The log-transformed data was filtered

for proteins present in at least 70% of all experiments. Significance filtering was based on

ANOVA testing, using FDR threshold of 0.01 with Benjamini Hochberg correction. In order to

perform PCA analysis and classification missing values were imputed by normal distribution.

Data shown in heatmap was Z-score normalized. Perseus output tables were transferred into

ClustVis [36] for visualization of hierarchical clustering and principle compound analysis (PCA).

Gene Ontology and functional analysis was performed via String DB (version 11.0.0) [37] and

Panther DB (version 14.1) [38]. For Panther DB analysis background genome was the human

genome and the total of identified proteins from all LC-MSMS runs in the experiments

(supplementary material 4-8). Feature optimization cross validation type was "n-fold" with n =

6. Kernel was either linear or RGF. All other settings were left on their default value.

Results:

In this study we investigated the utility of mass spectrometry-based methods for histo-molecular profiling applications in clinical renal cancer pathology. We analyzed thin tissue/tumor sections from three different renal cancer types (ccRCC, RO, ChRCC) by MALDI MS imaging and by an optimized rapid LC-MS/MS workflow adjusted to suit the demands for clinical settings.

Imaging by MALDI mass spectrometry

All samples were prepared as 5 µm thin FFPE tissue/tumor sections. The entire FFPE tissue section was analyzed by imaging MALDI MS imaging (MSI). The data was subsequently processed by unsupervised clustering (spatial shrunken centroid clustering [32]). The clustering results **(Figure 1A and 1B)** illustrate the heterogeneity of the tissue sections coming from various tissue types such as stroma, fibrotic fatty or healthy tissue and the capabilities of imaging MSI for the delineation of cancerous and non-cancerous tissue. Furthermore, when comparing the tumor area of the HE-stain/microscopy with the results from the mass spectrometry imaging based clustering, spectral differences even within the tumor tissue itself can be observed (**Figure 1A and 1C**).

Guided by the unsupervised clustering outcome and the corresponding image obtained by HE-staining, pixels from non-relevant surrounding tissue were discarded and only pixel clusters containing actual tumor tissue were used for subsequent comparative analyses (schematic workflow overview can be found in supplementary material: Figure S2).

In mass spectrometry imaging, principal component analysis (PCA) is often used for initial analysis of a given data set. Variance and similarities within the image sample set were estimated by PCA over the first 3 components. From a pathology viewpoint RO and ChRCC are more difficult to distinguish than ccRCC and ChRCC. As the sample holder for the imaging experiments can only hold 2 slides at a time, we first compared two conditions in a pairwise manner: 9 ccRCC vs. 9 RO **(Figure 2A)** and 5 RO vs. 5 ChRCC **(Figure 2B)**. Then the data set was combined to compare all three cancer conditions (9 ccRCC, 9 RO, 5 ChRCC) to each other **(Figure 2C).** PCA using the first three principle components separate ccRCC well from RO and ChRCC (**Figure 3A, 3C).** Data points from ccRCC showed a wide spread and were splitting into 2 sub-populations. In contrast, the data from RO and ChRCC samples cluster in a much tighter manner and with some overlap **(Figure 3A, 3B, 3C)**. This is particularly the case when considering all three cancer types together (**Figure 3C)**. When compared in a pairwise manner RO and ChRCC show slight separation **(Figure 3B)** suggesting at least some degree of histo-molecular differences between these cancer types. Some overlapping data points in the different cancer type datasets can be observed indicating histo-molecular spectral similarity in parts of the patient tumor tissues. The spread of ccRCC data points in PCA, as compared to the RO and ChRCC subtypes, suggests a greater heterogeneity among the ccRCC patient samples (also observed by LC-MS/MS, see later section).

Next, we assessed the ability of the MSI data to distinguish and classify renal cancer subtypes. We generated a classifier based on partial least squares discriminant analysis (PLS-DA) that can then be applied to a given MSI sample set. Due to the limited number of

FFPE kidney tumor samples we chose to use a cross-validation strategy that maximizes the

use of a sample set for model generation and testing. In this approach a classifier is trained

with imaging data from all samples, except for one sample that is set aside. As this sample is

not part of the classifier model it can then be used for testing purposes. This was repeated as

many times as there are samples ultimately allowing for testing the complete dataset (for n

samples we obtain n classifiers and n tested samples).

The optimized PLS-DA model resulted in an accuracy of cancer subtype prediction of 93% for

ccRCC and 88% for RO and for ChRCC. Results of the cross-validation study using PLS-DA

to classify 23 kidney tumor samples are depicted in **Figure 3**. The PLS-DA prediction scores

for each of the three possible tumor type outcomes are shown, i.e. ccRCC, RO and ChRCC.

The scores obtained for each pixel are presented by intensity scaled colors plotted over the

respective x-y-coordinate of the tissue/tumor sections.

Twenty of the 23 patient tumor samples were correctly assigned by the PLS-DA model

showing highest intensity for the respective cancer condition **(Figure 3)**. Eight out of nine

ccRCC samples were correctly assigned **(Figure 3a-i).** The PLS-DA classification provided

high scores for ccRCC samples and clearly distinguished the ccRCC samples from the other

two kidney tumor types (Figure 3, left panels). This is in accordance with the PCA results.

Likewise, the PLS-DA model provided low scores for ccRCC in the cases of RO and ChRCC

samples (Figure 3, middle and right panel). One ccRCC sample was incorrectly classified by

PLS-DA as RO **(Figure 3g)**.

All 5 ChRCC samples (**Figure 3 j-n**) were correctly assigned having the highest score for the

ChRCC condition (right panel). PCA indicated mass spectral similarities between the RO and

ChRCC samples. Likewise, the PLS-DA model reflects such similarities in the classification

outcome. Two ChRCC patient samples received highest scores for ChRCC but only slightly

lower scores for RO (**Figure 3k, 3n**). Furthermore, in the case of two RO sample the

classification could exclude ccRCC as diagnosis but was not able to further provide clear

information on if the cancer type in question is RO or ChRCC **(Figure 3a, 3e)**.

One kidney tumor sample (Figure 3l) exhibited a rather unusual scoring pattern as compared

to the other tumor samples. This particular sample received high scores for both ccRCC and

ChRCC classification (ChRCC being the highest). As mentioned above, we typically observed

clear distinction between ccRCC and ChRCC in all the other cases. Upon further pathology

and microproteomics analysis this tumor section was re-classified as a sarcomatoid

transformation (see below), i.e. a tumor type not included in the PLS-DA model used for

classification.

The relative importance of individual histo-molecular features of the classifier can be

visualized by plotting the PLS coefficients for each condition as a function of m/z values

(Figure 4). A positive coefficient indicates presence or higher abundance of the m/z value in

the respective cancer model. A negative coefficient indicates absence or lower abundance in

the respective condition. For ccRCC the two highest-ranking m/z values were m/z=723.5 and

m/z=704.5. The two highest values for RO were m/z=806.5 and m/z=1640.0 whereas the

most influential signals for ChRCC comprised m/z= 1169.5 and m/z=1039.5 (A top 100 list of

the features can be found in **supplementary material 2).** Unfortunately, we were not able to

obtain informative MALDI MS/MS fragment ion spectra in order to reveal the identity of these

peptide ion signals. Nevertheless, for classification purposes the knowledge of distinct

protein/peptide identities (m/z values) is not necessary as long as the signal is characteristic

for the tested condition.

In conclusion mass spectrometry imaging provided histo-molecular tumor profiles that can be

used to distinguish renal cancer subtypes. However, the misclassification of one ccRCC

patient and uncertainty of two additional diagnosis outcomes suggested that additional

independent test methods would be beneficial for confident classification of renal cancer

tumor types.

LC-MS/MS based rapid proteome profiling of tumor sections.

MALDI MS imaging provides spatial resolution that is helpful to address molecular

heterogeneity in tissue sections. However, MALDI MS imaging lacks analytical depth due to

the limited dynamic range of MALDI TOF MS and the poor performance of MALDI MS/MS for

protein identification by peptide sequencing directly from tissue sections. Deeper insight into

the tissue and tumor histo-molecular profiles and their variance will provide more diagnostic

features. We therefore adapted and optimized a microproteomics approach, combining *in situ*

protein sample preparation with fast proteome profiling by solid-phase extraction LC-MS/MS.

First a miniaturized *in situ* sample preparation method was applied where a small droplet of

trypsin solution is placed directly onto the tumor area of interest within a thin tissue section.

After overnight incubation the digested protein extract from the tumor area is subsequently

recovered and analyzed by mass spectrometry [39]. We reduced the LC-MS/MS analysis time

from 90 minutes to 15 min by using short LC gradients and rapid MS/MS functions, allowing

for a sample throughput of up to 80 samples per day. A total of 125 *in situ* extracted areas

from renal tumor sections were analyzed. Two to six *in situ* extracts were taken from each

renal tumor sample (11 RO sections from 11 patients: 47 extraction spots; 12 ccRCC sections

from 12 patients: 49 extraction spots; 7 ChRCC sections from 5 patients: 29 extraction spots).

Fast LC-MS/MS based microproteomics analysis of all 125 *in situ* digested tumor areas

resulted in a total of 2124 identified human proteins. We filtered the data for proteins that

were present in at least 70 % of all samples thereby reducing the protein number to 412

proteins. Comparative data analysis was performed for proteins that were significantly altered

(FDR=0.01) in any of the renal cancer subtypes resulting in a list of 346 differentially

regulated proteins. We then used unsupervised hierarchical clustering and PCA to identify

similarities and differences between the tumor samples. The x-axis dendrogram of the

heatmap shows that the majority of the renal tumor samples grouped according to cancer

subtype RO, ccRCC or ChRCC **(Figure 5A)**. Several large clusters of "co-regulated" proteins

are evident on the y-axis dendrogram and heatmap for the individual cancer subtypes. This

clearly demonstrates that there are renal cancer subtype specific histo-molecular features and

patterns in the microproteomics dataset.

The protein expression profiles of the three renal cancer subtypes are different based on the

heatmap patterns. ccRCC clearly differs from RO and ChRCC (**Figure 5A**: Protein group 2

and 4). RO and ChRCC display some differences but generally exhibit a more similar

expression pattern (**Figure 5A**: Protein Group 2).

These differences and similarities were also revealed by PCA analysis of the microproteomics

dataset. RO and ChRCC separate clearly from ccRCC (**Figure 5B)**. RO and ChRCC

datapoints are located close together, indicating that differences between the RO and ChRCC

cancer subtypes are less dominant. When considering principal components exhibiting less

variance (PC3 and PC4), separation of RO and ChRCC sample data is observed (**Figure**

5B).

We observed eight ChRCC proteomics datasets that separated clearly form the other ChRCC

datasets, both in hierarchical clustering analysis (**Figure 5A**) and PCA (**Figure 5B**). The

protein expression profile of these 8 samples exhibited some similarities to both ChRCC and

ccRCC. Interestingly, this data originated from a tumor from a single patient. This was the

same patient that also exhibited outlier MSI data with similarities to both ChRCC and ccRCC

tumor types, as discussed above (Figure 3I). Further pathology analysis revealed that these

samples were sarcomatoid renal cancer, originating from ChRCC and, thus, indeed different

from the other ChRCC samples.

Protein differences in cancer subtypes

Hierarchical clustering of the proteomics datasets revealed major differences in relative

protein abundance between the three renal cancer tumor types. (**Figure 5A**). We investigated

the nature of these histo-molecular differences by examining the correlation of these proteins

to cellular structures, functions, or biochemical processes. Protein groups that exhibited

distinctive abundances for the respective cancer type (**Figure 5:** ccRCC: group 1 & 4, RO:

group 2, ChRCC: group 3) were searched for their involvement in protein interaction networks

(supplementary material 9) as well as for their functional roles by using gene ontology (GO)

enrichment (**Figure 6**, supplementary material 3-8). We compared GO enrichment relative to

the experimental gene background comprising all genes corresponding to all 2124 identified

proteins in the LC-MSMS experiments (Figure 6, experimental background: blue) and the

complete human genome (Figure 6, human genome background: red).

RO and ChRCC exhibited a set of upregulated proteins (**Figure 5A**, *protein group 2)* that

were enriched for mitochondria associated proteins (GO:0005739), including various ATP

synthase subunits. Enriched protein functions comprised *oxidative phosphorylation*

(hsa00190), *citrate cycle* (hsa00020), and *fatty acid beta oxidation* (GO:0006635).

ChRCC-specific regulated proteins (**Figure 5A**, *protein group 3*) included cytoplasmic

proteins (GO:0044444), and proteins associated with *cytoplasmic vesicles* (GO:0031982) and

ribonucleoprotein complexes (GO:1990904).

Subtype-specific protein groups in ccRCC (**Figure 5A**, *protein group 1, 4*) were functionally

enriched for *complement activation* (GO:0006956), *regulation of blood coagulation*

(GO:0030193) and *platelet degranulation* (GO:0002576). Functions of *protein group 4* were

linked with *extra cellular matrix organization* (GO:0043062) and *cytoskeletal binding*

(GO:0008092) including proteins *collagen* and *laminin*. We also found several proteins such

as *glyceraldehyde-3-phosphate dehydrogenase* associated with the *glycolytic process*

(GO:0006096).

These functionally important findings can be correlated to known biochemical and

morphological features of each of the renal cancer subtypes. It is an established fact that the

number of mitochondria is increased dramatically in RO and ChRCC tumors (e.g. increased

oxidative phosphorylation) [40]. It is also known that ccRCC contains a highly vascularized

stroma (complement, coagulation, etc.) and exhibits a strong Warburg effect (glycolysis) [41].

Large intracellular vesicles are found in ChRCC (cytoplasmic proteins, vesicle proteins) [40].

Classification

Unsupervised data analysis demonstrated the presence of renal cancer subtype specific

differences in the tumor protein profiles. Next, we investigated the feasibility of tumor

classification by using the microproteomics data to train a prediction algorithm. We

implemented the tumor classification model by using a support vector machine (SVM)

approach. We chose the k-fold cross validation strategy [42] ("n-fold" in Perseus). Here the data

is randomly distributed in k groups. The model was then trained with data from k-1 groups

and the prediction was applied to the samples in the remaining group. This was repeated k

times. Low k-values tend to overestimate error rates. In our study 2-6 extraction spots

(samples) were derived from an FFPE section from each patient so too high k-values could

underestimate the true error rate. We therefore tested the prediction rate error over several k-

values (**Figure 7 A**) applying Radial Basis Function (RBF) and linear kernel functions [43]. The

tested error rates were in the range of 3.2% (4 wrong predictions) at the highest (k=3, linear

kernel) and 0 % at the lowest. However, k=3 is a very low k-value (excluding more than 41

samples from the training set). We argue that the error rate is most likely overestimated in this

case. For more commonly used k-values (k=5-10) the error rate was between 0.8% (1 wrong

prediction) and 0% for RBF and 1.6% (2 wrong prediction) and 0% for linear kernel function.

Incorrectly predicted outcomes included samples from one RO patient predicted as ccRCC.

Generally, RBF performed slightly better than linear kernel. Figure 7B exemplifies the

outcome of the cross-validation resulted for RBF and k=6 (around 20 samples per group

equivalent to 4 patients excluded from the training set). Each sample was scored for the three

tested conditions (ccRCC, RO, ChRCC). The highest scoring condition was used to classify a

given sample. Results are shown in a radar plot (**Figure 7B**) and demonstrate 100% accuracy

in prediction of renal cancer subtypes.

As mentioned previously, one renal tumor was initially incorrectly classified and was indeed a

ChRCC derived sarcomatoid renal tumor. The computational classification methods used

here cannot classify anything, which has not been previously "taught" to the system. In the

particular case of the sarcomatoid patient samples this means that they will be classified as

one of the three cancer types ccRCC, ChRCC or RO. Interestingly despite the similarity to

ccRCC (**Figure 5B**) the sarcomatoid patient samples were predicted by our SVM as ChRCC.

This is in accordance with their cancer type origin prior transformation.

We initially used all 346 differentially abundant histo-molecular features (proteins) to classify

the tumor subtypes. Next, we sought to estimate the minimum number of features that suffice

to correctly classify all the renal tumor samples (for k=6 and RBF). We used the feature

optimization function in the Perseus software, which first ranks the features and then tests the

error rate for a decreasing number of features (**Figure 7C**). The minimal number out of the

346 features was found to be 43 features (list of the ranked proteins can be found in supplementary material 9). Further reducing the number to 21 features resulted in an error rate of 1.6% and as little as 6 features lead to an error rate of 9.6%. Conclusively only a portion of the dataset, i.e. at least 43 features would suffice to successfully classify all the kidney tumor samples. However, keeping an excess of quantified protein features would be beneficial as "safety margin" assuring a high enough number of quantified protein features for robust classification of tumors.

Data integration from MSI and rapid proteome profiling

Having both MSI and microproteomics sets of data at hand provides several advantages for classification of cancer tumor FFPE samples. Using the MSI approach for tumor classification we observed a higher error rate than with the rapid micro-proteomics approach. In two cases MSI could exclude one cancer type but was not providing clear results towards an RO or a ChRCC diagnosis. Another case where one ccRCC sample was misclassified as RO is particularly problematic as ccRCC might need surgery whereas RO does not. Therefore, by integrating the micro-proteomics classification data the outcome of the MSI classification can be further confirmed, clarified or rejected (**Table 1**). This allows more confidence in diagnosis or could possibly even provide further information on cancer stage or treatment strategies. In a case where the classification model does not cover the cancer condition such as in the patient sample with sarcomatoid transformation we have demonstrated how irregularities and inconsistencies are detected by both MSI and rapid LC-MS/MS based microproteomics (**Figure 3I, 5A, 5B**). This provides an opportunity to further investigate, refine and expand the range of computational and statistical classification models.

An additional application making use of the combined data set includes the investigation of

histo-molecular properties observed in MSI (e.g. intra- tumor heterogeneity) by correlation to

information from the rapid microproteomics approach. Usually a detailed investigation of MSI

feature data is achieved by either microproteomics "in situ protein digestion" or laser

microdissection based approaches [44] using LC-MS/MS based proteomics analysis with long

LC gradient times (1-4 hours). Despite the shorter gradient times and thus lower protein

coverage in the here presented approach the information can nevertheless be used to

investigate histo-molecular properties observed in MSI to a certain degree (e.g. intra- tumor

heterogeneity). We exemplified this in Figure 8, using the RO MSI data set previously shown

(Figure 1, top). Unsupervised clustering of MSI data revealed two distinct regions within the

tumor area (Figure 8: cluster 1 and cluster 2). Correlating the LC-MSMS data from the

respective extraction spots within these distinct regions in deed reveals significant differential

abundances of in 80 proteins (the protein list can be found in supplementary material 11).

Hierarchical clustering of these 80 proteins with regard to their extraction position correlates

well with the distinct regions depicted by the MSI clustering (MSI Cluster 2 correlates with

extraction spots E-F, MSI Cluster 2 correlates with extraction spots A-D; Figure 8). The

proteomics data suggests a lower abundance of mitochondrial associated proteins and a

higher abundance in some cytoskeletal protein binding proteins in cluster 2. The area

comprising Cluster 2 located on the edge of the tumor and might indicate the differences that

can be encountered between the inner and outer tumor regions [45].

Discussion

The increasing incidence of renal cancer in western countries calls for improved technologies

for detection, diagnosis, treatment and prognosis. Innovative mass spectrometry-based

applications are beginning to address challenges in clinics and the healthcare sector, such as

the use of targeted proteomics to characterize noninvasive liquid biopsies [46] or the so called

iKnife, enabling surgeons to identify cancerous tissue in real time [47,48]. Mass spectrometry is

becoming increasingly applicable in a clinical setting [49,50]. FFPE sections are a valuable

source for mass spectrometry-based diagnosis. As many of the sample preparation steps for

MS analysis overlap with the preparation steps for (immuno)histochemical staining, they can

be seamlessly fit into the high-throughput sample preparation pipeline for FFPE sections

(deparaffination, antigen retrieval) already existing in many hospitals. Distinguishing

numerous cancer types or subtypes and making decisions for treatment modalities are daily

challenges in hospitals. Approaches that include "digital" large-scale data acquisition and

computer-based machine learning algorithms provide deep molecular insight into the

respective disease and provides valuable information for early detection, diagnostic and

prognostic purposes.

Our proof of concept study demonstrates the potential and benefits of mass spectrometry

techniques for detailed characterization of clinical specimen. Specifically, we demonstrate

that mass spectrometry provides valuable results in the diagnosis of different renal cancer

subtypes (ccRCC, RO and ChRCC). The imaging mass spectrometry (MSI) approach allows

to collect spatially resolved spectra without *a priori* knowledge of the tissue, thereby enabling

the differentiation between cancerous and noncancerous tissue, as well as subtyping of

tumors. In our study MALDI-MSI could correctly diagnose 20 out of 23 of the tested patients.

In two of the 3 misclassified cases it was however possible to narrow down the diagnosis to

either RO or ChRCC. Despite the promising results the misclassification of a ccRCC sample

as RO might be problematic as RO may not require surgery but ccRCC does. Both cases

stress how using rapid proteome profiling data in parallel provides additional confidence and

can help avoid a false negative prognosis.

The MSI PCA data showed that the patient-to-patient tumor variability is significant for

ccRCC, necessitating a detailed histo-molecular profile for robust MSI performance. The

inclusion of many more patients (n>100) to increase the number of renal cancer tumor

samples will likely provide higher confidence and could resolve this issue.

Microproteomics analysis by in situ protein digestion in FFPE sections combined with

optimized and rapid LC-MS/MS based protein identification and quantification correctly

classified all the tested renal tumor samples in cross validation experiments. The efficient

peptide separation and sequencing capability of modern LC-MS/MS provided deeper insight

into the renal cancer proteome than possible by the MSI approach alone. The higher

dimensionality of the many protein features revealed by microproteomics improved the SVM

based prediction and achieved 100% accurate classification of renal cancer subtypes in cross

validation experiments.

Notably, unsupervised clustering identified data inconsistencies and irregularities in the

patient cohort. An unexpected feature pattern revealed a sarcomatoid transformation within

the ChRCC cohort, without *a priori* knowledge (**Figure 5A, 5B**). This goes to demonstrate that

once the "digital" data is acquired then the computational and statistical applications can

uncover relevant and important features of the patient datasets. This sensitivity, specificity

and versatility will have major implications for future clinical practices, including histo-

molecular pathology technologies.

The presented microproteomics method based on optimized, fast chromatographic separation

and fast MS/MS sequencing of peptides identified more than 2100 proteins in thin renal tumor

FFPE sections. Using short LC runs of only 15 min. we generated a list of 346 significantly

altered proteins (p=0.01). The minimum number of proteins determined to be necessary for

100% accurate tumor classification was 43. This low number of features enables a targeted

proteomics approach aimed at quantifying a select panel of proteins. Using fewer features

would also allow a further reduction of LC run time and increase overall sample throughput.

Using our fast LC-MS/MS setup we analyzed a total of 125 samples in a series without

experiencing blocking of the LC columns, glass capillaries or ESI needles. LC systems such

as the EvoSep system [25] that are specifically dedicated for clinical applications and tailored to

be used also by non LC-MS experts can add additional robustness to our approach.

Furthermore, implementation of image pattern recognition guided pipetting robots may

enhance reproducibility and throughput, e.g. using liquid extraction surface analysis (LESA)

technology [51,52]. The latter has been successfully applied in the study of traumatic brain

injuries [53] as well as in mouse brain for the identification of proteins and peptides from MSI

experiments [54]. The missing value problem is still a common problem in label free quantitative

proteomics. Successful implementation of protein identification on MS1 level only has been

presented recently [55] and could be interesting to following up in the here presented context in

future experiments.

Functional protein analysis using bioinformatics tools revealed molecular networks and

biochemical processes consistent with previously known macroscopic, morphological and

histological features of the renal cancer subtypes. Cancer-type specific proteome expression

features correlated to morphological characteristics of the respective cancer type. RO and

ChRCC exhibited upregulation of mitochondrial associated proteins. Indeed, increased

numbers of mitochondria are frequently observed in these cancer types by electron

microscopy [56] and have been identified in previous proteomics studies [57]. As most cancer rely

on glycolysis as major energy source (Warburg effect) this seems rather unusual. However,

those mitochondria are malfunctioning and it has been speculated that increase in number of

mitochondria is a cellular response to the presence of dysfunctional mitochondria [58].

In addition to mitochondria associated proteins increased intracytoplasmic associated

proteins were detected in ChRCC distinguishing it from the other cancer types.

Microscopically, ChRCC is distinguished from other renal carcinomas by its pale cytoplasm

resulting from large intracytoplasmic vesicles. This accounts for our detection of an increase

of intracellular cytoplasm-associated proteins and vesicle proteins, distinguishing ChRCC

from the other two renal tumor subtypes RO and ccRCC.

Clear cell renal cell carcinoma frequently contains zones of hemorrhage that are most likely

responsible for the increased levels of complement and coagulation cascade associated

proteins, as determined by our microproteomics method. ccRCC is also characterized by

hypervascular stroma [3], which may account for the enrichment of extracellular matrix proteins.

Again, enhanced glycolysis is a hallmark of many cancer types including ccRCC [41] correlating

well with our detection of upregulated glycolysis associated proteins by microproteomics.

For classification we applied PLS-DA to MSI data and support vector machine to the LC-

MSMS data. These common classification methods have previously been applied to MSI for

the differentiation of papillary and renal cell carcinoma based on lipidomics analysis [59] as well

as for the classification of epithelial ovarian cancer subtypes [16]. There are, however,

numerous other classification methods available. Mascini *et al.* used principal component

linear discriminant analysis in order to predict treatment response in xenograft models of

triple-negative breast cancer [60]. Recently, deep convolutional networks were proposed [61].

Both MSI and short gradient LC-MS/MS microproteomics methods come with their individual

advantages. Applying both approaches in parallel for routine analysis is most beneficial to

improve confidence in diagnosis and identify irregularities. In order to create very robust

classifiers for use in clinical settings the promising results of this study need to be further

supported in the future by analysis of larger patient cohorts.

With the enormous progress in sample handling and instrument technology, machine learning

[62] and the availability of new databases [63] mass spectrometry is on its way to become a

versatile tool in the hospital clinics of the future.

Acknowledgements

Proteomics and mass spectrometry research at SDU are supported by generous grants to the

VILLUM Center for Bioanalytical Sciences (VILLUM Foundation grant no. 7292 to O.N.J.) and

PRO-MS: Danish National Mass Spectrometry Platform for Functional Proteomics (grant no.

5072-00007B to O.N.J.). We thank Veit Schwämmle and Livia Rosa Fernandes for advice

and discussion on the project.

Authors Contributions:

U.M., O.N.J. and N.M. planned and outlined the project. N.M. provided the patient samples

and patient diagnosis. U.M. performed all experiments and data analysis. U.M. and O.N.J.

wrote the manuscript.

Competing Interests:

The Authors declare no competing interest

References

Bray, F. *et al.* Global cancer statistics 2018: GLOBOCAN estimates of incidence and mortality worldwide for 36 cancers in 185 countries. *CA Cancer J Clin* **68**, 394-424, doi:10.3322/caac.21492 (2018).

Jonasch, E., Gao, J. & Rathmell, W. K. Renal cell carcinoma. *BMJ* **349**, g4797, doi:10.1136/bmj.g4797 (2014).

Muglia, V. F. & Prando, A. Renal cell carcinoma: histological classification and correlation with imaging findings. *Radiol Bras* **48**, 166-174, doi:10.1590/0100-3984.2013.1927 (2015).

Ng, K. L. *et al.* Differentiation of oncocytoma from chromophobe renal cell carcinoma (RCC): can novel molecular biomarkers help solve an old problem? *J Clin Pathol* **67**, 97-104, doi:10.1136/jclinpath-2013-201895 (2014).

Carella, R. *et al.* Immunohistochemical panels for differentiating epithelial malignant mesothelioma from lung adenocarcinoma: a study with logistic regression analysis. *Am J Surg Pathol* **25**, 43-50 (2001).

Angelidis, I. *et al.* An atlas of the aging lung mapped by single cell transcriptomics and deep tissue proteomics. *Nat Commun* **10**, 963, doi:10.1038/s41467-019-08831-9 (2019).

Clark, A. E., Kaleta, E. J., Arora, A. & Wolk, D. M. Matrix-assisted laser desorption ionization-time of flight mass spectrometry: a fundamental shift in the routine practice of clinical microbiology. *Clin Microbiol Rev* **26**, 547-603, doi:10.1128/CMR.00072-12 (2013).

Kriegsmann, M. *et al.* Detection of HPV subtypes by mass spectrometry in FFPE tissue specimens: a reliable tool for routine diagnostics. *J Clin Pathol* **70**, 417-423, doi:10.1136/jclinpath-2016-204017 (2017).

Ellis, S. R. *et al.* Automated, parallel mass spectrometry imaging and structural identification of lipids. *Nat Methods* **15**, 515-518, doi:10.1038/s41592-018-0010-6 (2018).

Hannes Hinneburg, P. K., Falko Schirmeister, Slavko Gasparov, Peter & H. Seeberger, V. Z., Daniel Kolarich. Spatial glycomics of histopathological formalin-fixed and paraffin embedded (FFPE) tissue microdissections. *Molecular & Cell Proteomics* **in review** (2016).

Moginger, U. *et al.* Alterations of the Human Skin N- and O-Glycome in Basal Cell Carcinoma and Squamous Cell Carcinoma. *Front Oncol* **8**, 70, doi:10.3389/fonc.2018.00070 (2018).

Caprioli, R. M., Farmer, T. B. & Gile, J. Molecular imaging of biological samples: localization of peptides and proteins using MALDI-TOF MS. *Anal Chem* **69**, 4751-4760, doi:10.1021/ac970888i (1997).

Stoeckli, M., Farmer, T. B. & Caprioli, R. M. Automated mass spectrometry imaging with a matrix-assisted laser desorption ionization time-of-flight instrument. *J Am Soc Mass Spectrom* **10**, 67-71, doi:10.1016/S1044-0305(98)00126-3 (1999).

Casadonte, R. *et al.* Development of a Class Prediction Model to Discriminate Pancreatic Ductal Adenocarcinoma from Pancreatic Neuroendocrine Tumor by MALDI Mass Spectrometry Imaging. *Proteomics Clin Appl* **13**, e1800046, doi:10.1002/prca.201800046 (2019).

Mascini, N. E., Teunissen, J., Noorlag, R., Willems, S. M. & Heeren, R. M. A. Tumor classification with MALDI-MSI data of tissue microarrays: A case study. *Methods* **151**, 21-27, doi:10.1016/j.ymeth.2018.04.004 (2018).

Klein, O. *et al.* MALDI-Imaging for Classification of Epithelial Ovarian Cancer Histotypes from a Tissue Microarray Using Machine Learning Methods. *Proteomics Clin Appl* **13**, e1700181, doi:10.1002/prca.201700181 (2019).

Mallah, K. *et al.* Lipid Changes Associated with Traumatic Brain Injury Revealed by 3D MALDI-MSI. *Anal Chem* **90**, 10568-10576, doi:10.1021/acs.analchem.8b02682 (2018).

18 Briggs, M. T. *et al.* MALDI mass spectrometry imaging of N-glycans on tibial cartilage and subchondral
bone proteins in knee osteoarthritis. *Proteomics* **16**, 1736-1741, doi:10.1002/pmic.201500461 (2016).
19 Perkins, D. N., Pappin, D. J., Creasy, D. M. & Cottrell, J. S. Probability-based protein identification by
searching sequence databases using mass spectrometry data. *Electrophoresis* **20**, 3551-3567,
doi:10.1002/(SICI)1522-2683(19991201)20:18<3551::AID-ELPS3551>3.0.CO;2-2 (1999).
20 Eng, J. K., McCormack, A. L. & Yates, J. R. An approach to correlate tandem mass spectral data of
peptides with amino acid sequences in a protein database. *J Am Soc Mass Spectrom* **5**, 976-989,
doi:10.1016/1044-0305(94)80016-2 (1994).
21 Zhao, M. *et al.* A Comparative Proteomics Analysis of Five Body Fluids: Plasma, Urine, Cerebrospinal
Fluid, Amniotic Fluid, and Saliva. *Proteomics Clin Appl* **12**, e1800008, doi:10.1002/prca.201800008
(2018).
22 Schmidt, A. & Aebersold, R. High-accuracy proteome maps of human body fluids. *Genome Biol* **7**, 242,
doi:10.1186/gb-2006-7-11-242 (2006).
23 Eliuk, S. & Makarov, A. Evolution of Orbitrap Mass Spectrometry Instrumentation. *Annu Rev Anal Chem*
(Palo Alto Calif) **8**, 61-80, doi:10.1146/annurev-anchem-071114-040325 (2015).
24 Falkenby, L. G. *et al.* Integrated solid-phase extraction-capillary liquid chromatography (speLC)
interfaced to ESI-MS/MS for fast characterization and quantification of protein and proteomes. *J*
Proteome Res **13**, 6169-6175, doi:10.1021/pr5008575 (2014).
25 Krieger, J. R. *et al.* Evosep One Enables Robust Deep Proteome Coverage Using Tandem Mass Tags
while Significantly Reducing Instrument Time. *J Proteome Res* **18**, 2346-2353,
doi:10.1021/acs.jproteome.9b00082 (2019).
26 Horning, O. B., Kjeldsen, F., Theodorsen, S., Vorm, O. & Jensen, O. N. Isocratic solid phase extraction-
liquid chromatography (SPE-LC) interfaced to high-performance tandem mass spectrometry for rapid
protein identification. *Journal of proteome research* **7**, 3159-3167, doi:10.1021/pr700865c (2008).
27 Hørning O. B. , T. S., Vorm O., Jensen O. N. Solid phase extraction-liquid chromatography (SPE-LC)
interface for automated peptide separation and identification by tandem mass spectrometry.
International Journal of Mass Spectrometry **268,**, 147-157, doi:10.1016/j.ijms.2007.06.017. (2007).
28 Stoeckli, M., Staab, D., Wetzel, M. & Brechbuehl, M. iMatrixSpray: a free and open source sample
preparation device for mass spectrometric imaging. *Chimia (Aarau)* **68**, 146-149,
doi:10.2533/chimia.2014.146 (2014).
29 Kovalchuk, S. I., Jensen, O. N. & Rogowska-Wrzesinska, A. FlashPack: Fast and Simple Preparation of
Ultrahigh-performance Capillary Columns for LC-MS. *Molecular & cellular proteomics : MCP* **18**, 383-
390, doi:10.1074/mcp.TIR118.000953 (2019).
30 Rompp, A. *et al.* imzML: Imaging Mass Spectrometry Markup Language: A common data format for
mass spectrometry imaging. *Methods in molecular biology* **696**, 205-224, doi:10.1007/978-1-60761-
987-1_12 (2011).
31 Bemis, K. D. *et al.* Cardinal: an R package for statistical analysis of mass spectrometry-based imaging
experiments. *Bioinformatics* **31**, 2418-2420, doi:10.1093/bioinformatics/btv146 (2015).
32 Bemis, K. D. *et al.* Probabilistic Segmentation of Mass Spectrometry (MS) Images Helps Select
Important Ions and Characterize Confidence in the Resulting Segments. *Molecular & cellular*
proteomics : MCP **15**, 1761-1772, doi:10.1074/mcp.O115.053918 (2016).
33 Wold, S., Sjostrom, M. & Eriksson, L. PLS-regression: a basic tool of chemometrics. *Chemometr Intell*
Lab **58**, 109-130, doi:Doi 10.1016/S0169-7439(01)00155-1 (2001).
34 Cox, J. & Mann, M. MaxQuant enables high peptide identification rates, individualized p.p.b.-range
mass accuracies and proteome-wide protein quantification. *Nat Biotechnol* **26**, 1367-1372,
doi:10.1038/nbt.1511 (2008).

35   Tyanova, S. *et al.* The Perseus computational platform for comprehensive analysis of (prote)omics data.
Nat Methods **13**, 731-740, doi:10.1038/nmeth.3901 (2016).
36   Metsalu, T. & Vilo, J. ClustVis: a web tool for visualizing clustering of multivariate data using Principal
Component Analysis and heatmap. *Nucleic acids research* **43**, W566-570, doi:10.1093/nar/gkv468
(2015).
37   Szklarczyk, D. *et al.* STRING v11: protein-protein association networks with increased coverage,
supporting functional discovery in genome-wide experimental datasets. *Nucleic acids research* **47**,
D607-D613, doi:10.1093/nar/gky1131 (2019).
38   Thomas, P. D. *et al.* PANTHER: a library of protein families and subfamilies indexed by function.
Genome Res **13**, 2129-2141, doi:10.1101/gr.772403 (2003).
39   Wisztorski, M. *et al.* Microproteomics by liquid extraction surface analysis: application to FFPE tissue to
study the fimbria region of tubo-ovarian cancer. *Proteomics Clin Appl* **7**, 234-240,
doi:10.1002/prca.201200070 (2013).
40   **John. Eble, L. C.** in *Modern Surgical Pathology (Second Edition)* (ed Richard J. Cote Noel Weidner, Saul
Suster, Lawrence M. Weiss) 1043-1078 (W.B. Saunders, 2009).
41   Courtney, K. D. *et al.* Isotope Tracing of Human Clear Cell Renal Cell Carcinomas Demonstrates
Suppressed Glucose Oxidation In Vivo. *Cell Metab* **28**, 793-800 e792, doi:10.1016/j.cmet.2018.07.020
(2018).
42   Hastie, T., Tibshirani, R. & Friedman, J. in *The Elements of Statistical Learning: Data Mining, Inference,*
and Prediction   219-259 (Springer New York, 2009).
43   Hastie, T., Tibshirani, R. & Friedman, J. in *The Elements of Statistical Learning: Data Mining, Inference,*
and Prediction   191-218 (Springer New York, 2009).
44   Dewez, F. *et al.* Precise co-registration of mass spectrometry imaging, histology, and laser
microdissection-based omics. *Analytical and bioanalytical chemistry* **411**, 5647-5653,
doi:10.1007/s00216-019-01983-z (2019).
45   Oppenheimer, S. R., Mi, D., Sanders, M. E. & Caprioli, R. M. Molecular analysis of tumor margins by
MALDI mass spectrometry in renal carcinoma. *Journal of proteome research* **9**, 2182-2190,
doi:10.1021/pr900936z (2010).
46   Kim, Y. *et al.* Targeted proteomics identifies liquid-biopsy signatures for extracapsular prostate cancer.
Nature Communications **7**, doi:ARTN 11906

10.1038/ncomms11906 (2016).
47   Phelps, D. L. *et al.* The surgical intelligent knife distinguishes normal, borderline and malignant
gynaecological tissues using rapid evaporative ionisation mass spectrometry (REIMS). *Br J Cancer* **118**,
1349-1358, doi:10.1038/s41416-018-0048-3 (2018).
48   Schafer, K. C. *et al.* In vivo, in situ tissue analysis using rapid evaporative ionization mass spectrometry.
Angew Chem Int Ed Engl **48**, 8240-8242, doi:10.1002/anie.200902546 (2009).
49   Heaney, L. M., Jones, D. J. & Suzuki, T. Mass spectrometry in medicine: a technology for the future?
Future Sci OA **3**, FSO213, doi:10.4155/fsoa-2017-0053 (2017).
50   Longuespee, R., Casadonte, R., Schwamborn, K. & Kriegsmann, M. Proteomics in Pathology: The Special
Issue. *Proteomics Clin Appl* **13**, e1800167, doi:10.1002/prca.201800167 (2019).
51   Wisztorski, M. *et al.* Spatially-resolved protein surface microsampling from tissue sections using liquid
extraction surface analysis. *Proteomics* **16**, 1622-1632, doi:10.1002/pmic.201500508 (2016).
52   Wisztorski, M. *et al.* Droplet-Based Liquid Extraction for Spatially-Resolved Microproteomics Analysis of
Tissue Sections. *Methods Mol Biol* **1618**, 49-63, doi:10.1007/978-1-4939-7051-3_6 (2017).

53 Mallah, K. *et al.* Mapping Spatiotemporal Microproteomics Landscape in Experimental Model of
Traumatic Brain Injury Unveils a link to Parkinson's Disease. *Mol Cell Proteomics* **18**, 1669-1682,
doi:10.1074/mcp.RA119.001604 (2019).
54 Ryan, D. J. *et al.* Protein identification in imaging mass spectrometry through spatially targeted liquid
micro-extractions. *Rapid communications in mass spectrometry : RCM* **32**, 442-450,
doi:10.1002/rcm.8042 (2018).
55 Ivanov, M. V. *et al.* DirectMS1: MS/MS-Free Identification of 1000 Proteins of Cellular Proteomes in 5
Minutes. *Analytical chemistry* **92**, 4326-4333, doi:10.1021/acs.analchem.9b05095 (2020).
56 Thoenes, W., Storkel, S. & Rumpelt, H. J. Human chromophobe cell renal carcinoma. *Virchows Arch B*
Cell Pathol Incl Mol Pathol **48**, 207-217, doi:10.1007/bf02890129 (1985).
57 Drendel, V. *et al.* Proteomic distinction of renal oncocytomas and chromophobe renal cell carcinomas.
Clin Proteomics **15**, 25, doi:10.1186/s12014-018-9200-6 (2018).
58 Gasparre, G., Romeo, G., Rugolo, M. & Porcelli, A. M. Learning from oncocytic tumors: Why choose
inefficient mitochondria? *Biochimica et biophysica acta* **1807**, 633-642,
doi:10.1016/j.bbabio.2010.08.006 (2011).
59 Dill, A. L. *et al.* Multivariate statistical differentiation of renal cell carcinomas based on lipidomic
analysis by ambient ionization imaging mass spectrometry. *Anal Bioanal Chem* **398**, 2969-2978,
doi:10.1007/s00216-010-4259-6 (2010).
60 Mascini, N. E. *et al.* The use of mass spectrometry imaging to predict treatment response of patient-
derived xenograft models of triple-negative breast cancer. *Journal of proteome research* **14**, 1069-
1075, doi:10.1021/pr501067z (2015).
61 Behrmann, J. *et al.* Deep learning for tumor classification in imaging mass spectrometry. *Bioinformatics*
34, 1215-1223, doi:10.1093/bioinformatics/btx724 (2018).
62 Jordan, M. I. & Mitchell, T. M. Machine learning: Trends, perspectives, and prospects. *Science* **349**, 255-
260, doi:10.1126/science.aaa8415 (2015).
63 Gessulat, S. *et al.* Prosit: proteome-wide prediction of peptide tandem mass spectra by deep learning.
Nat Methods **16**, 509-518, doi:10.1038/s41592-019-0426-7 (2019).

Figure 1

Figure 2

Figure 3

757   **Figure 4:**

Figure 5

Figure 6

767 **Figure 7**

A

B

Predicted: ccRCC	Predicted: ChRCC	Predicted: RO	T: True group
49	0	0	True: ccRCC
0	29	0	True: ChRCC
0	0	47	True: RO

C

Figure 8

776 **Table 1**

Pathologist diagnosis	Patient	MSI diagnosis	Rapid LC-MSMS diagnosis	Conclusion
RO	42839	RO/ChRCC	RO	RO
RO	23119	RO	RO	RO
RO	49527	RO	RO	RO
RO	9270	RO	RO	RO
RO	11529	RO/ChRCC	RO	RO
RO	55560	RO	RO	RO
RO	49940	RO	RO	RO
RO	56857	RO	RO	RO
RO	3381	RO	RO	RO
ccRCC	18427	ccRCC	ccRCC	ccRCC
ccRCC	17370	ccRCC	ccRCC	ccRCC
ccRCC	10620	ccRCC	ccRCC	ccRCC
ccRCC	16073	ccRCC	ccRCC	ccRCC
ccRCC	12545	ccRCC	ccRCC	ccRCC
ccRCC	14999	ccRCC	ccRCC	ccRCC
ccRCC	17797	RO	ccRCC	ccRCC/further validation
ccRCC	8601	ccRCC	ccRCC	ccRCC
ccRCC	10336	ccRCC	ccRCC	ccRCC
ChRCC	47638	ChRCC	ChRCC	ChRCC
ChRCC	6835	ChRCC	ChRCC	ChRCC
ChRCC	21264*	ChRCC with irregularities	ChRCC with irregularities	further validation -> sarcomatoid transformation
ChRCC	58756	ChRCC	ChRCC	ChRCC
ChRCC	39925	ChRCC	ChRCC	ChRCC

Table 1: integrated testing strategy for classification of renal cancer types. Initial pathologist diagnosis and patient number are indicated in the first 2 columns. *Patient sample showed irregularities and after reassessment could be diagnosed as sarcomatoid transformation. Concluding contradictory results would either necessitate further validation or the outcome of the more reliable method (LC-MSMS) could be favored

Figure 1 Tumor sample heterogeneity is revealed by mass spectrometry imaging and unsupervised clustering. A) Spatial Shrunken centroid clustering of ccRCC and RO data obtained by imaging mass spectrometry of ccRCC and RO tissue sections. Based on differences and similarities in the spectra each pixel was automatically assigned a certain cluster (indicated by a different color). B) Average MALDI mass spectra of the respective tumor areas (histo-molecular clusters) reveal distinct features and individual variations in the m/z signals. C) HE-stain of tumor tissue section from same FFPE block. Tumor area is indicated in red.

Figure 2: 3D PCA score plot from imaging MALDI MS experiments of kidney tumor tissues. Each plot contains the extracted pixel data from all patients of a given cancer type. Data from ccRCC (A) (magenta) and ChRCC (B) (blue) are compared to RO (yellow). (C) Data from all three cancer types are compared to each other. The graph displays the first 3 principle components (PC1, PC2, PC3) plotted against each other. Clear separation of data points between ccRCC and RO can be observed by pairwise comparison but also in the combined

comparison to both RO and ChRCC. In pairwise comparison (B) RO and ChRCC show slight

separation but exhibit a great number of overlapping features. ccRCC exhibits the largest

differences to RO and ChRCC. RO and ChRCC appear to share more spectral similarities.

Figure 3: Tumor classification by MALDI MS imaging and cross-validation using PLS-DA

classification. Pixels/spectra from tumor areas only, were extracted for processing.

Classification of 9 ccRCC and 9 RO (a-i) sample as well as 5 RO sample and 5 ChRCC

sample (j-n). Pathology diagnosis of the respective patient samples are indicated to the left

and right of the images (*RO, ccRCC* or *ChRCC*). Each spectrum-containing pixel is predicted

individually. The prediction scores are represented by a color scale. Each cancer condition

was tested and scored so that each sample set is represented in 3 panels. Each of the panels

displays scores for ccRCC (first panel) RO (second panel) and ChRCC (third panel) The

respective testing condition is indicated on top above the panels. (Cardinal´s smooth.image-

function was used for better visibility. Unprocessed image can be found in supplementary

material 1 Figure S4)

Each sample is predominantly predicted in the correct diagnosis, achieving accuracies (pixel-

based value) of 93% (ccRCC), 88% (RO), 88% (ChRCC). Winner of the classification is

marked with a green bar for correct classification and a red bar for incorrect classification.

Figure 4: PLS coefficients as a function of *m/z*. The diagram displays the impact of each

detected *m/z* signal feature in imaging MS data from PLS-DA prediction (spectra are binned

to 0.25 m/z bins). Positive coefficient indicates presence or higher abundance in the

respective condition. Negative coefficient indicates absence or lower abundance of the m/z

value in the respective condition (a list with the 100 most influential features can be found in

supplementary material 2)

Figure 5: Unsupervised renal cancer subtype classification by microproteomics using rapid

LC-MS/MS protein profiling. A) Heatmap and hierarchical clustering of differential relative

protein abundances. Columns indicate samples and rows indicate proteins. The renal cancer

subtype of the patient sample is indicated in colored bars on top. The graph shows the large

similarities in protein expression profiles among patient samples with the same cancer

subtype causing them to cluster together. Furthermore, hierarchical clustering of the protein

abundances reveals protein cluster that are detected in a cancer subtype specific manner.

Protein groups selected for subsequent network analysis are indicated by color blocks on the

y-axis dendrogram (groups 1-4). B) Principal component analysis of the sample set. Dotted

ellipses are such that with a probability of 95% a new observation from the same group will

fall inside the area. The first (PC1) and second (PC2) component explain 17.6 % of the total

variance whereas the other components lie at 7.7% and 4.4% respectively. There is a clear

separation of ccRCC and RO samples already in the first two principal components.

Differences between RO and ChRCC are subtle and are only evident when considering

components that display lower variance (PC2:PC3 and PC3:PC4). The small group of the

eight ChRCC-derived sarcomatoid renal cancers samples cluster relatively far from the other

ChRCC samples, thereby identifying these as clear "outliers" that require further attention.

Figure 6: Bioinformatics analysis (PantherDB) identified enriched biochemical functions in

renal tumors. Protein groups were compared against a background of all the 2124 proteins

identified in the experiment (blue) and against the background of the human genome (red).

Fold enrichment (increase over expected value) as well as -log of the false discovery rate

(FDR) are shown.

Figure 7: Microproteomics and SVM model correctly classifies all renal tumor subtypes. A)

Dependency of the classification error rate in relation to increasing k-value. RBF performs

slightly better than the linear kernel function. From value k=4 and higher, error rates vary

between 0% and 0.8% (1 wrong prediction out of 125) for RBF and between 0% - 1.6 % for

linear kernel. B) Radar plot of the cross-validated classification (k=6, kernel=RBF) of

proteome profiles obtained from each tumor section extraction spot. Scores for each of the

three tumor types are displayed. Scores range from lowest (center) to highest (outer circle).

The highest score indicates highest likelihood for the respective diagnosis. (Scores for

ccRCC: magenta, ChRCC: yellow, RO: blue). The pathological diagnosis for each sample is

indicated on the outside of the radar plot. The plot shows that all samples score highest in

correlation with the respective cancer type indicating the high accuracy of the classification.

C) Feature optimization. The error rate for linear kernel and RBF are plotted over the number

of ranked features (proteins).   Decreasing feature number results in increase of false

predictions. Minimum number of features for 0% error rate is at 43 using RBF and 86 for

linear kernel (list of ranked proteins can be found in supplementary material 10).

Figure 8: Combined use of MS imaging and rapid LC-MSMS microproteomics provides histo-molecular details of tumor heterogeneity. A) MSI based unsupervised clustering analysis of a RO patient sample. Two clusters (cluster 1 and cluster 2) are detected within the tumor area. Positions used for extraction of LC-MSMS samples are indicated by red circles extractions A-F (2 extractions for cluster 1, 4 extractions in cluster 2).

B) Volcano plot of LC-MSMS data derived ratio of protein abundance (Cluster 2 / Cluster1). Proteins with significant (t-test: $p=0.01$, 2-fold difference) different abundances are colored in blue.

C) Heatmap display of the significantly different proteins from extraction spots A-F. On the x-axis extraction spots A-D and E-F group together. The grouping is in correlation to the MSI clustering data. On the y axis two protein groups can be observed distinguishing the two x-axis-cluster. One group is upregulated in Cluster 1 the other group is upregulated in Cluster 2.

D) StringDB network analysis of upregulated proteins in MSI-Cluster-2 (top, sample: A-D) and upregulated proteins in MSI-Cluster 1 (bottom, sample: E-F). Cluster 2 shows higher abundance of mitochondrial associated proteins whereas cluster 1 shows increase abundance of cytoskeletal protein binding proteins.