Temporal context actively shapes EEG signatures of time perception

Atser Damsma[1*], Nadine Schlichting[1], Hedderik van Rijn[1]

[1]Department of Psychology, University of Groningen, Grote Kruisstraat 2/1, 9712 TS, Groningen, the

Netherlands

[*]Corresponding author: Atser Damsma (a.damsma@rug.nl)

Abstract

Our subjective perception of time is optimized to temporal regularities in the environment. This is illustrated by the central tendency effect: when estimating a range of intervals, short intervals are overestimated whereas long intervals are underestimated to reduce the overall estimation error. Most models of interval timing ascribe this effect to the weighting of the current interval with previous memory traces *after* the interval has been perceived. Alternatively, the *perception* of the duration could already be flexibly tuned to its temporal context. We investigated this hypothesis using an interval reproduction task in which human participants (both sexes) reproduced a shorter and longer interval range. As expected, reproductions were biased towards the subjective mean of each presented range. EEG analyses showed that temporal context indeed affected neural dynamics during the perception phase. Specifically, longer previous durations decreased CNV and P2 amplitude and increased beta power. In addition, multivariate pattern analysis showed that it is possible to decode context from the transient EEG signal quickly after both onset and offset of the perception phase. Together, these results suggest that temporal context creates dynamic expectations which actively affect the *perception* of duration.

Keywords: time perception; context; Bayesian perception; EEG

Significance Statement

The subjective sense of duration does not arise in isolation, but is informed by previous experiences. This is demonstrated by abundant evidence showing that the production of duration estimates is biased towards previously experienced time intervals. However, it is yet unknown whether this temporal context actively affects perception or only asserts its influence in later, post-perceptual stages as proposed by most current formal models of this task. Using an interval reproduction task, we show that EEG signatures flexibly adapt to the temporal context during perceptual encoding. Furthermore, interval history can be decoded from the transient EEG signal even when the current duration was identical. Thus, our results demonstrate that context actively influences perception.

Introduction

The way humans experience time is not only driven by the current stimulus, but is also

influenced by previous experiences. According to Bayesian observer models, humans integrate noisy

sensory representations (the likelihood) with previously learned stimulus statistics (the prior

distribution). This is illustrated by the temporal context or central tendency effect: when presented

with a range of intervals, short intervals are overestimated and long intervals are underestimated

(Jazayeri & Shadlen, 2010). Furthermore, the prior distribution has been shown to be dynamically

updated, such that more recent intervals have a greater influence on the current estimate (Dyjas,

Bausenhart, & Ulrich, 2012; Taatgen & van Rijn, 2011; Wiener, Thompson, & Branch Coslett, 2014).

Although there is abundant behavioral evidence for Bayesian integration in human time perception

(Acerbi, Wolpert, & Vijayakumar, 2012; Cicchini, Arrighi, Cecchetti, Giusti, & Burr, 2012; Gu,

Jurkowski, Lake, Malapani, & Meck, 2015; Hallez, Damsma, Rhodes, van Rijn, & Droit-Volet, 2019;

Jazayeri & Shadlen, 2010; Maaß, Riemer, Wolbers, & van Rijn, 2019; Maaß, Schlichting, & van Rijn,

2019; Roach, McGraw, Whitaker, & Heron, 2017; Schlichting et al., 2018; Shi, Church, & Meck,

2013), its temporal locus and neural underpinnings are not yet understood.

Computational models of interval timing often (implicitly) assume that only after perception

has completed, the noisy interval percept is weighted with previous memory traces representing the

prior (e.g., Di Luca & Rhodes, 2016; Jazayeri & Shadlen, 2010; Taatgen & van Rijn, 2011).

Alternatively, however, prior experience might actively affect perception, as evidenced by recent

behavioral (Cicchini, Benedetto, & Burr, 2020; Cicchini, Mikellidou, & Burr, 2017; Zimmermann &

Cicchini, 2020), fMRI (St. John-Saaltink, Kok, Lau, & De Lange, 2016) and single neuron findings

(Sohn, Narain, Meirhaeghe, & Jazayeri, 2019). Specifically, Sohn et al. (2019) showed that neurons in

the prefrontal cortex of monkeys exhibited different firing rate patterns based on the prior during

interval estimation.

In humans, evidence is now emerging that electroencephalography (EEG) signatures in

timing tasks are modulated by recently perceived durations. In a bisection task, longer prior durations

led to a larger amplitude of the contingent negative variation (CNV) and increased beta oscillations

power (Wiener, Parikh, Krakow, & Coslett, 2018; Wiener & Thompson, 2015). Crucially, however,

these studies required an active comparison to the standard interval, in which EEG signatures have

been shown to reflect an adjustment of the decision threshold (Ng, Tobin, & Penney, 2011; see also

Boehm, Van Maanen, Forstmann, & van Rijn, 2014). Any context-based changes in these signatures

might reflect updating of the comparison process. It is therefore still an open question what the

temporal locus of the context effect is: Does the prior exert its influence in post-perceptual stages or

are purely perceptual processes already affected by previous experiences?

We tested the influence of temporal context in an interval reproduction task, which allowed us

to distill EEG signals during the perception phase in which no decision or motor response was

required that could yield fallacious conclusions regarding the effect of context effects during

perception. Participants reproduced two different interval ranges (the *short* and the *long context*). The

ranges shared one interval (the *overlapping interval*), providing a condition in which the physical

stimulus was the same, but the temporal context was different. We show that temporal context affects

three EEG signatures that have previously been associated with time perception during the perception

phase: the CNV and beta oscillations, but also the offset P2, which has been shown to predict

subjective interval perception better than the CNV (Kononowicz & van Rijn, 2014; Kruijne, Olivers,

& van Rijn, 2021). A data-driven approach reveals that temporal context can be decoded from

transient neural dynamics during the perception phase using multivariate pattern analysis (MVPA).

Together, these results show that temporal context actively shapes the perception of duration,

falsifying most current formal theories of interval timing.

73   **Materials and Methods**

Participants

Twenty-seven healthy adults (22 females; age range 18 - 33 years, $M = 21.33$, $SD = 3.78$

years) participated in the experiment for course credits in the University of Groningen Psychology

program or monetary compensation (€ 14). Two participants were excluded from analysis during pre-

processing due to excessive artifacts in the EEG data. The study was approved by the Psychology

Ethical Committee of the University of Groningen (17141-S-NE). Written informed consent was

obtained before the experiment. After the experiment, the participants were debriefed about the aim of

the study.

Stimuli and apparatus

Stimuli were presented using the Psychophysics Toolbox 3.0.12 (Brainard, 1997; Kleiner et

al., 2007) in Matlab 2014b. Intervals were presented as continuous 440 Hz sine wave tones. These

auditory stimuli were presented on Sennheiser HD 280 Pro stereo headphones at a comfortable sound

level. Visual stimuli were presented in the center of the screen in Helvetica size 25 in white on a dark

grey background using a 27-inch Iiyama ProLite G27773HS monitor with a 1920x1080 resolution at

100 Hz. The index-finger trigger buttons of a gamepad (SideWinder Plug & Play Game Pad,

Microsoft Corporation) were used to record responses.

Procedure

Participants performed an auditory interval reproduction task (Figure 1A). Every trial started

with a central fixation cross with a uniform random duration between 2 and 3 s. Then, an exclamation

mark was presented for 0.7 s, after which the auditory interval was presented (the *perception phase*)

while the exclamation mark remained on the screen. To signal the next phase, the exclamation mark

was replaced by a question mark which was presented for 1.5 s. Next, the continuous tone was

presented again, with the question mark remaining on the screen, which participants had to terminate

by pressing a button (the *reproduction phase*). Participants were instructed to match the duration of

this second tone to the duration of the first tone as accurately as possible.

The task involved two different interval ranges, the short context (0.625 s, 0.75 s, and 0.9 s)

and the long context (0.9 s, 1.08 s, and 1.296 s) (Figure 1A). Crucially, there was an *overlapping*

interval that was presented in both contexts (0.9 s). The experiment consisted of four blocks, two of

which used intervals of the short context, and two of which used intervals of the long context. Block

order was counterbalanced across participants, with the constraint that the context would alternate

every block. Within a block, each duration of the short or the long context was presented 30 times,

amounting to a total of 90 trials per block and 360 trials over the whole experiment. The presentation

order was random, with the constraint that every possible subsequent pair of intervals was presented

equally often (i.e., first-order counterbalancing). The hand needed for reproduction was switched after

Figure 1. Task and behavioral results. A) Behavioral procedure of the experiment. Participants performed an interval reproduction task in which they heard a tone for a certain duration (*perception phase*). After an ISI of 1.5 s, they were asked to reproduce this duration by pressing a button to indicate the offset of the *reproduction phase*. In separate blocks, the perception phase consisted of three short or three relatively long durations (the *short* and the *long context*, respectively). One interval was presented in both contexts (the *overlapping interval* of 0.9 s). B) Average behavioral reproduction results. Error bars represent the standard error of the mean. C) Average reproduction of the overlapping interval (0.9 s) for the different intervals in the previous trial, relative to average reproduction in the context condition. Overall, reproductions were longer when the prior interval was longer. D) Link between the EEG signatures and reproductions. The left panel shows the reproduction of the overlapping interval for relatively low, medium, and high values (i.e., tertiles) of the CNV amplitude, P2 amplitude, P2 latency, and beta power. The right panel shows the correlation between participants' behavioral context effect and their context effect in the different EEG signatures (all values were *z*-scored). Dots represent individual participants, while the lines represent linear regression lines.

two blocks. Prior to each block, participants were instructed which hand (i.e., which gamepad button)

they would use to terminate the duration and which set of intervals would be presented (termed set A

and set B for the short and long context, respectively; see also Maaß, Schlichting, et al., 2019), while

they were not informed about the relative durations or distributions associated with the sets (i.e., that

the sets were associated with a short and long interval range). Participants could take self-timed

breaks between blocks. Prior to the experiment, participants performed two practice trials with

durations outside the range of both context conditions (0.4 s and 2 s). Experiment scripts are available

at https://osf.io/sgbjz/.

EEG acquisition

EEG signals were recorded from 62 Ag/AgCl electrodes, placed in accordance with the

international 10-20 system (WaveGuard EEG cap, eemagine Medical Imaging Solutions GmbH,

Berlin, Germany). The ground electrode was placed onto the left side of the collarbone and the

mastoids served as location for the reference electrodes. The electrooculogram (EOG) was recorded

from the outer sides of both eyes and from the top and bottom of the left eye. Data was collected at a

sampling frequency of 512 Hz using a TMSi Refa 8-64 amplifier. Before the experiment, impedances

of all electrodes were reduced to below 5kΩ. Participants were instructed to blink only between trials

and not to move during the experiment.

EEG pre-processing

EEG pre-processing was performed using the FieldTrip toolbox (Oostenveld, Fries, Maris, &

Schoffelen, 2011). EEG data was re-referenced to the averaged mastoids and filtered using a

Butterworth IIR band-pass filter with a high-pass frequency of 0.01 Hz and a low-pass frequency of

80 Hz. Subsequently, trial epochs were created from -1 s until 6 s relative to the onset of the

perception phase. Artifacts were corrected using independent component analysis (ICA). Epochs that

exceeded an amplitude range of 120 μV were removed from the dataset. On average, 10.72% ($SD =$

6.10) of the 360 trials were discarded.

Data Analysis

Behavioral analysis. Reproductions lower than 0.1 s and higher than 2 s were excluded from

analysis (0.2% of the data). To test whether reproductions were influenced by context, we fitted a

linear mixed model (LMM) using the *lme4* package (Bates, Mächler, Bolker, & Walker, 2015) in R

(R Core Team, 2016), including interval, context, their interaction and prior interval (i.e., the interval

in the previous trial) as fixed factors. To facilitate interpretation of the results, interval and prior

interval were centered at 0.9 s and the factor context was recoded using effect coding (-0.5 for short

and 0.5 for long context). In addition to the random intercept of participant, we sequentially added

random slope terms and tested whether they improved the model with a likelihood ratio test. We will

here report the results of the best fitting model, which included random slopes for interval and prior

interval.

ERP analysis. All EEG analyses reported here focused on the perception phase. An overview

of the EEG results in the reproduction phase is available in the supplementary materials (section 1) at

https://osf.io/sgbjz/. The CNV and beta signatures in the reproduction phase show trends that are

qualitatively similar to the perception phase, although they appear to be less strong.

CNV. The CNV analysis was performed on a fronto-central electrode cluster (electrodes Cz,

C1, C2, FCz, FC1, FC2) (Kononowicz & van Rijn, 2014; Ng et al., 2011). A 10 Hz Butterworth low-

pass filter was applied and the ERP was baselined to the average signal in the 0.1 s window before

interval onset. To test the effect of global context during the perception phase, we compared the ERP

of the overlapping interval in the short and the long context using a cluster-based permutation test

(Maris & Oostenveld, 2007) in the window 0-1.2 s from interval onset. The permutation test assessed

whether the difference was different from zero by computing 100.000 permutations using the *t*-

statistic, controlling for multiple comparisons with a cluster significance threshold of $p < .05$. To

assess the influence of the prior interval on CNV, we calculated the average amplitude in the time

window that showed CNV differences in the previously mentioned permutation test (0.3-1.01 s), per

participant, context and prior interval for the overlapping interval. Next, we tested an LMM predicting

this amplitude, including context and prior interval as fixed factors, and participant as a random

intercept term.

Offset P2. The P2 analysis focused on the EEG signal averaged over the same fronto-central

electrode cluster as the CNV analysis, to which a 1–20 Hz Butterworth band-pass filter was applied to

minimize CNV-based contamination (cf., Kononowicz & van Rijn, 2014). The ERP was baselined to

the average signal in the 0.1 s window around interval offset (cf., Kononowicz & van Rijn, 2014).

Similar to the CNV analysis, the ERPs of the overlapping interval in the short and the long context

were compared using a cluster-based permutation test in the window 0-0.5 s after interval offset.

Next, we calculated P2 amplitude was as the average amplitude between 0.14 and 0.3 s after interval

offset (this window was based on Kononowicz & van Rijn, 2014). We fitted an LMM predicting P2

amplitude, with interval, prior interval, and context as fixed factors, and participant as a random

intercept term. The random slope of interval improved the fit and was added to the model. P2 latency

was calculated as the 50% area latency - the time point at which half of the area under the curve is

reached - within the same window (Liesefeld, 2018; Luck, 2005). P2 latency was analyzed using an

LMM with the same fixed factors as the P2 amplitude model.

Because the 1 Hz high-pass filter might induce artifactual effects of opposite polarity before

the actual peak (Tanner, Morgan-Short, & Luck, 2015), we also performed the P2 analysis on the data

without additional filtering (that is, besides the band-pass filter between 0.01 Hz and 80 Hz applied

during pre-processing). We found similar qualitative results, which are reported in the supplementary

materials section 2.1 at https://osf.io/sgbjz/.

Multivariate pattern analysis. To investigate transient neural dynamics in more detail, we

tested whether it is possible to decode global and local context through MVPA of the EEG signal.

Following Wolff, Kandemir, Stokes, and Akyürek (2020), we used a sliding window approach in

which the EEG fluctuations were pooled over electrodes and time. A window of 50 data points (98

ms) was moved across the signal in steps of 8 ms, separately for each channel. Within the window, the

signal was down-sampled to 10 samples (by taking the average over 5 samples) and baseline-

corrected by subtracting the mean within the window from all 10 individual samples.

To decode whether an overlapping-interval trial was presented in the short or the long

context, the 10 samples per electrode in each time window served as input for 5-fold cross-validation.

In each fold, we calculated the Mahalanobis distance (De Maesschalck, Jouan-Rimbaud, & Massart,

2000; Wolff, Jochim, Akyürek, & Stokes, 2017; Wolff et al., 2020) between the test trials and the

averaged signal of the short and long context, using the covariance matrix estimated from the training

trials with a shrinkage estimator (Ledoit & Wolf, 2004). To make the distance estimates more reliable,

the 5-fold cross-validation was repeated 50 times and results were averaged. The eventual decoding

distances were smoothed with a Gaussian smoothing kernel ($SD = 16$ ms). To test whether the

distance between conditions was significantly different from zero, a cluster-based permutation test

was performed.

A similar analysis was performed to decode the duration of the prior interval from the neural

dynamics in the current trial. For the overlapping interval, the Mahalanobis distance between every

test trial and the average of the prior interval conditions was calculated. This resulted in six difference

time series for each condition (including the 0.9 s condition for each context separately and the

difference with the trial's own condition). In this way, we aimed to determine whether the distance

was higher when the difference between the prior interval condition of the test trial and the other

possible prior interval conditions was larger. Next, for every time point, we performed a linear

regression on the Mahalanobis distance, using the absolute difference between prior interval

conditions (in seconds) and the difference between context (coded as 0 or 1) as predictors, allowing us

to disentangle the effect of sequential and global context on transient neural dynamics. A cluster-

based permutation test was performed on the resulting slope values for prior interval and context, to

test whether they deviated from zero (using a one-sided *t*-test).

To investigate which electrodes are most informative in decoding the context of an

overlapping interval trial, we performed channel-wise decoding: the procedure to decode global

context outlined above was performed separately for every electrode. Topographies were created to

show the average decoding accuracy at the different electrodes during time windows in which the

Mahalanobis distance resulting from the context decoding procedure outlined above (i.e., using all

electrodes) was significantly higher than zero.

Because the context conditions were blocked in our experimental design, the decoding

accuracy might have been inflated by nonstationarities in the EEG signals, which lead to stochastic

dependence between trials (Lemm, Blankertz, Dickhaus, & Müller, 2011). Post-hoc, we controlled for

this notion by calculating the Mahalanobis distance between the different blocks, for each participant.

This allowed us to differentiate between the distances between blocks that were presented in the first

and second half of the experiment, and thereby, to test whether the original decoding results could be

due to within-block similarities beyond context. In this way, we compared the Mahalanobis distance

between the trials in a particular block and the 'same context' and 'different context' block in the

other half of the experiment. We found that the results were qualitatively similar to the original

analysis, with significant differences between the short and long context immediately after interval

onset and after interval offset (analysis details and full results can be found in the supplementary

materials section 2.2. at https://osf.io/sgbjz/).

Time-frequency analysis. To assess oscillatory power during the perception phase we

performed a time-frequency analysis using a single Hanning taper with an adaptive time window of 6

cycles per frequency in steps of 15 ms for frequencies from 4 to 40 Hz, with the amount of spectral

smoothing set to 1. We calculated the absolute power from the baseline window of -0.2-0 s relative to

interval onset. The analysis was again focused on fronto-central electrodes (Cz, C1, C2, FCz, FC1,

FC2). Similar to the CNV analysis, all time-frequency analyses were performed on the overlapping

interval to isolate the effect of context while keeping the actual stimulus constant.

Per participant, for every time-frequency point, we fitted a linear regression model including

prior interval (a continuous variable ranging from the shortest to the longest interval in seconds) and

context (short and long context coded as 0 and 1, respectively) as predictors (following an approach

similar to Wiener et al., 2018). For every time-frequency point, this resulted in two slope values,

expressing the relative influence of the global context and the previous interval. Next, a one-sample *t*-

test against zero was performed for the two slope values at each time-frequency point, which was

corrected for multiple comparisons using cluster-based permutation (Maris & Oostenveld, 2007). The

statistical testing was performed on the frequency range of 8-30 Hz to include alpha power (8–14 Hz**;**

Kononowicz & van Rijn, 2015) and beta power (15–30 Hz; e.g., Haegens et al., 2011; Jenkinson &

Brown, 2011; Kononowicz & van Rijn, 2015) during the time window of 0-1.2 s after interval onset.

Linking EEG signatures and behavior. We tested in two ways whether EEG signatures

during the perception phase predicted behavioral reproductions. First, we computed *single trial* values

of CNV amplitude, P2 amplitude, P2 latency and beta power. Following the methods described above,

for every trial, CNV amplitude was calculated as the average EEG signal in the window 0.3-1.01 s

after interval onset, P2 amplitude as the average between 0.14 and 0.3 s after interval offset, P2

latency as the 50% area latency in the same window, and beta power was calculated as the average

power in the time window 0.48-0.84 s after interval onset and the frequency range 23-30 Hz, which

was based on the permutation test. CNV, P2 amplitude, P2 latency, and beta power values that

deviated more than 4 SD from the average were excluded from analysis (0.06%, 0.01%, 0.00% and

0.46% of the trials, respectively). Similar to the behavioral analysis described above, reproductions

shorter than 0.1 s and longer than 2 s were also excluded from analysis. Next, we computed four

LMMs with reproduction as the dependent factor, and CNV amplitude, P2 amplitude, P2 latency, and

beta power as fixed factors, respectively. Similar to the analyses described above, the CNV and beta

power analyses were focused on the overlapping interval trials. To control for the effect of context on

both EEG signatures and behavior, context and prior interval were also added as fixed factors to the

models. The P2 analysis included all intervals, so here, interval was entered as an additional fixed

factor. In all models, participant was included as a random intercept term, and adding random slopes

did not improve the model fit in any of the models.

261   Second, in addition to the single trial analysis, we looked at individual differences: Do

participants who show a large context effect in the EEG signatures also show a large behavioral

context effect? To this end, for the overlapping interval, we estimated the behavioral context effect

(i.e., the difference in reproduction between the long and short context) for each participant, and

compared it to the context effect of CNV amplitude, P2 amplitude and latency, and beta power,

quantified as described in the previous paragraphs. To assess whether these measures were related for

each participant, we performed a one-tailed Pearson's correlation test between the individual

behavioral context effects and the EEG context effects.

269   **Results**

270   **Behavioral results**

271   Figure 1B shows the average reproductions for the different intervals. The results of the LMM

showed that the reproductions increased with duration ($\beta = 0.77$, $SE = 0.03$, $t = 24.33$, $p < .001$). We

found a significant effect of global context, showing that reproductions were longer in the long

compared to the short context ($\beta = 0.05$, $SE = 0.01$, $t = 7.23$, $p < .001$). In addition, the increase with

duration (i.e., the slope) was lower for the long compared to the short context ($\beta = -0.18$, $SE = 0.03$, t

$= -7.01$, $p < .001$). Besides the global context effect, reproductions were longer when the interval in

the previous trial was longer ($\beta = 0.08$, $SE = 0.02$, $t = 3.41$, $p = .002$). Figure 1C shows the

reproductions for the different previous intervals, relative to the average reproduction.

ERPs

280   **CNV.** Figure 2A and 2B show the average fronto-central ERP during the perception phase for

281   the different intervals in the short and the long context, respectively. In addition, Figure 2D shows a

282   direct comparison between the short and the long context of this ERP for the overlapping interval (0.9

283   s). The cluster-based permutation test showed that the CNV was more negative in the short than in the

284   long context in the time windows 0.30-0.65 s ($p = .004$) and 0.71-1.01 s ($p = .003$). Thus, while the

Figure 2. Average ERPs at the fronto-central cluster (Cz, C1, C2, FCz, FC1, FC2) relative to the onset of the perception phase for the different durations in the short (A) and long (B) context. In all panels, vertical grey dashed lines indicate interval onset and offset of the overlapping interval (0.9 s). C) Topographies of the overlapping interval (0.9 s), for the short context, long context, and their difference, during the window of significant difference as indicated by the cluster-based permutation test. D) Average ERP of the overlapping interval (0.9 s) in the short and the long context. Grey horizontal bars indicate significant differences according to the cluster-based permutation test. E) Average ERP of the overlapping interval, split up according to the interval in the previous trial. Red and blue lines show whether the overlapping interval appeared in the short or the long context, respectively. F) Average CNV amplitude for the middle interval, in the time window of significant difference between the short and long context, for the different previous intervals. Error bars represent the standard error of the mean.

actual interval was the same, CNV amplitude during perception differed depending on the temporal

context.

Figure 2E shows the average ERP for the overlapping interval, split for the different previous

durations, and Figure 2F shows the average CNV in the 0.3-1.01 s window for the different prior

interval conditions. The LMM results showed that CNV amplitude at the overlapping interval became

less negative with longer previous trials (β = 2.50, SE = 0.97, t = 2.57, p = .011). There was no

evidence for an additional significant effect of context (β = 0.43, SE = 0.42, t = 1.03, p = .308),

suggesting that the global context effect on CNV might be largely driven by the previous trial. Post-

hoc, we tested whether including the interaction between context and prior interval improved the

model fit, but a likelihood ratio test showed that this was not the case ($\chi^2(1)$ = 0.10, p = .750).

Figure 3. Amplitude and latency of the P2 at the fronto-central cluster (Cz, C1, C2, FCz, FC1, FC2) after the offset of the perception phase. A, B) Grand average ERPs baselined at the offset of the perception phase in the short and the long context, respectively. C) Topographies of P2 amplitude of the overlapping interval (0.9 s), for the short context, long context, and their difference, during the window of significant difference as indicated by the cluster-based permutation test. D) Average ERP of the overlapping interval (0.9 s) in the short and the long context. Grey horizontal bars indicate significant differences according to the cluster-based permutation test. F) Effect of interval on P2 amplitude and latency. The left panel shows P2 amplitude, calculated as the average amplitude in the window 0.14-0.3 s after interval offset for every participant and interval. The right panel shows P2 latency, calculated as the 50% area latency in the same window. G) Effect of the prior interval on P2 amplitude (left) and latency (right). In all figures, error bars represent the standard error of the mean.

Offset P2. *Amplitude.* Figure 3A and 3B shows the offset P2 for the different intervals in the

short and the long context, respectively. Figure 3D directly compares the P2 for the overlapping

interval in the short and long context. The cluster-based permutation test showed that the amplitude

was higher for the short compared to the long context in the window 0.11-0.3 s. Figure 3F shows the

average P2 amplitude as a function of interval and context. The LMM showed that the P2 increased

with duration (β = 5.56, SE = 0.62, t = 8.97, p < .001), but that the intercept was significantly lower

for the long compared to the short context (β = -0.87, SE = 0.28, t = -3.10, p = .002). Figure 3E and

3G (left panel) show the effect of the prior interval on P2 amplitude for the overlapping interval. In

line with the global context effect, the model showed that the P2 decreased with longer previous

intervals (β = -1.71, SE = 0.51, t = -3.35, p = .001). Together, these results show that P2 amplitude

reflects the actual duration, as well as the global and local context in which the duration appeared.

Latency. Figure 3F (right panel) shows that P2 latency decreased with the duration of the

current interval, which was confirmed by the LMM predicting latency (β = -0.04, *SE* = 0.01, *t* = -3.66,

p < .001). There was no evidence that P2 latency was affected by the context, as the fixed factors

contex and prior interval did not reach significance (*p*s > .247). In summary, whereas P2 amplitude

reflects the current duration and the general and sequential temporal context, P2 latency only

decreases with longer current durations.

Multivariate pattern analysis

Figure 4A shows the decoding accuracy for the overlapping interval. The permutation test

showed a positive cluster immediately after interval onset (0-0.17 s; *p* = .009) and after interval offset

(0.99-1.37 s; *p* < .001). Figure 4C shows the topographies of the channel-wise decoding results during

these two clusters, which reflects high parietal and left-lateralized decoding accuracy and high fronto-

central and right-lateralized decoding accuracy, respectively. Figure 4B shows the slope value of prior

interval in the regression analysis predicting Mahalanobis distance. The permutation test showed that

there was no evidence for significant clusters for the slope of prior interval or context in the regression

analysis (*p* = .999), showing that MVPA could not distinguish between prior interval conditions based

on the transient EEG signal.

Figure 4. Decoding accuracy relative to the onset of the perception phase. A) Decoding accuracy of context for the overlapping interval as represented by the Mahalanobis distance. Grey horizontal bars indicate a significant difference from zero according to the cluster-based permutation test. Error shading represent 95% CI of the mean. B) Decoding accuracy of prior interval in the overlapping interval, represented by the slope value of the regression of Mahalanobis distance with prior interval and context as predictors. C) Topographies of channel-wise context decoding accuracy for the overlapping interval, during the first significant cluster in panel A (left) and the second cluster (right). Colors represent the decoding accuracy in Mahalanobis distance.

Time-frequency analysis

To assess oscillatory power during the perception phase, we calculated a linear regression of frequency power at fronto-central electrodes with context (short vs long) and prior interval as predictors for every time-frequency point during the overlapping interval. Figure 5A shows the slope values representing the effect of context on the power of the different frequencies over time. We found a positive cluster in the window 0.48-0.84 s after interval onset in the 23-30 Hz frequency range (p = .045), indicating increased beta power in the long context compared to the short context (see the outlined area in Figure 5A). This beta effect is further illustrated in Figure 3C, which shows the average power in the 23-30 Hz over time, for the overlapping interval in the short and long context. Figure 5B shows the slope values for prior interval, for which the permutation test indicated no evidence for a cluster of slopes different from zero (ps > .051). In summary, these results suggest that fronto-central beta power was higher in the long compared to the short context, while there was no evidence for a similar influence of the previous trial.

Figure 5. Slope values of regression on frequency power at fronto-central electrode cluster (electrodes Cz, C1, C2, FCz, FC1, FC2) relative to the onset of the perception phase. A) Slope values of the factor Context (short vs long) in the regression analysis at every time-frequency point. The outlined area marks a significant cluster according to the cluster-based permutation test performed in the time window 0-1.2 s and the frequency window 8-30 Hz. B) Slope values of the factor prior interval in the regression analysis predicting power. There was no evidence for significant clusters. In both panels, vertical dashed grey lines indicate the onset and offset of the perception phase. C) Average beta power in the time and frequency range of the significant cluster (23-30 Hz) for the short and long context for the overlapping interval. Error shading represents represent the standard error of the mean. D) Topographies of beta power for the overlapping interval, in the time and frequency range of the significant cluster, for the short context, the long context, and their difference.

Linking EEG signatures and behavior

Figure 1C shows the effect of single-trial EEG signatures on reproductions of the overlapping

interval. For illustration purposes, the single-trial EEG amplitudes and latencies were divided into

tertiles (low/short, medium, high/long) for each participant and context, and the average reproduction

was plotted for each tertile. The LMMs showed no evidence that single-trial CNV and beta power in

the perception phase predicted reproductions in the reproduction phase ($\beta = 0.0003$, $SE = 0.0004$, $t =$

0.85, $p = .395$ and $\beta = 0.0003$, $SE = 0.0019$, $t = -0.51$, $p = .614$, respectively). This was also the case

for P2 latency, with a trend towards shorter reproductions for later P2 peaks ($\beta = -0.08$, $SE = 0.04$, $t =$

-1.80, $p = .072$). However, P2 amplitude after perception phase offset was predictive of that trial's

reproduction ($\beta = -0.0010$, $SE = 0.0003$, $t = -3.45$, $p < .001$). As the β-value indicates, higher P2 peaks

were followed by shorter reproductions. Given that context, interval and prior interval were also

included as fixed factors in the LMM, these results cannot be attributed to a mediating influence of

context, and therefore suggest that trial-by-trial variation in P2 amplitude might be a reliable predictor

of reproductions.

We additionally tested whether participants with a large behavioral context effect for the

overlapping interval also showed a large context effect in the EEG signatures. This between-

participant relationship between these measures is depicted in Figure 1D. Analysis showed that the

individual behavioral context effect was correlated with the P2 amplitude difference between contexts

($r(23) = -.37$, $p = .033$). We found no evidence for a similar relationship with P2 latency ($r(23) = -.18$,

$p = .196$), CNV amplitude ($r(23) = .19$, $p = .180$) or beta power ($r(23) = -.22$, $p = .861$). Thus, in line

with the single trial analysis, P2 amplitude differences predict reproduction outcomes.

356   **Discussion**

As the temporal locus of Bayesian computations in human time estimation is still unknown,

we investigated whether temporal context actively influences neural signatures during the perception

of time intervals. Behaviorally, we found that reproductions were biased towards the global temporal

context as well as the duration in the previous trial. EEG results showed that CNV, P2 and beta power

were modulated by previously perceived intervals, and that context could be decoded from transient

brain dynamics at an early stage during perception. These results indicate that previously perceived

durations actively affect EEG signatures during interval estimation, showing that prior experiences act

directly on perception. This observation goes against the (implicit) assumption of time perception

models that the likelihood is weighted with the prior only after perception. It is, however, in line with

recent behavioral evidence showing that context asserts its influence at early sensory stages (Cicchini

et al., 2020; Zimmermann & Cicchini, 2020). Our findings suggest that experiences with the global

and recent temporal context actively calibrate cortical dynamics, in which the CNV and beta power

may reflect the anticipation of stimulus duration, and the P2 component the active evaluation of the

interval in the current context. Crucially, by focusing on the perception phase in a reproduction

paradigm, this is the first work demonstrating context effects that are not linked to explicit motor

preparation or response decisions.

Our findings argue against the idea that the CNV reflects the neural counterpart of the

absolute accumulator in pacemaker-accumulator models (Casini & Vidal, 2011; Macar & Besson,

1985; Macar & Vidal, 2004; Macar, Vidal, & Casini, 1999; Macar & Vitton, 1982; Pfeuty, Ragot, &

Pouthas, 2005), since no differences based on prior experience would be expected during the

perception of an interval. Instead, we found that the CNV during the perception of the overlapping

interval was more negative for the short compared to the long context, and for shorter previous

durations. This is consistent with anticipation and preparation accounts of the CNV (e.g., Boehm et

al., 2014; Elbert, 1993; Leuthold, Sommer, & Ulrich, 2004; Mento, 2013; Ng et al., 2011; Scheibe,

Schubert, Sommer, & Heekeren, 2009) and pacemaker-accumulator models that propose adaptive

spike rate accumulation (Simen, Balci, deSouza, Cohen, & Holmes, 2011): When interval offset is

expected quickly after onset, CNV amplitude increases more rapidly. This adaptation is in line with

studies showing a faster CNV development for relatively short foreperiods (Miniussi, Wilding, Coull,

& Nobre, 1999; Müller-Gethmann, Ulrich, & Rinkenauer, 2003; Trillenberg, Verleger, Wascher,

Wauschkuhn, & Wessel, 2000; Van der Lubbe, Los, Jaśkowski, & Verleger, 2004), shorter standard

durations in an interval comparison task (Pfeuty et al., 2005), and after adaptation to a shorter interval

(Li, Chen, Xiao, Liu, & Huang, 2017). The contextual adjustment of the speed with which the CNV

develops suggests that neural populations in the supplementary motor area (SMA), which is typically

associated with the CNV (e.g., Coull, Vidal, & Burle, 2016), can perform flexible temporal scaling

based on the temporal context (Remington, Egger, Narain, Wang, & Jazayeri, 2018; Remington,

Narain, Hosseini, & Jazayeri, 2018; Sohn et al., 2019), even in the absence of explicit motor

preparation. The prior might calibrate the speed of neural dynamics through different initial states at

the onset of the perception phase (Remington, Egger, et al., 2018; Sohn et al., 2019), as our

multivariate pattern analysis showed that global context can be decoded from EEG dynamics

immediately after the onset of the perception phase. Although the precise onset of significant

decoding should be interpreted with caution since the moving window approach and low-pass filtering

could smear out the accuracy over time (Grootswagers, Wardle, & Carlson, 2017), these results

suggest that temporal context affects the instantaneous neural response to to-be-timed stimuli.

400   The active anticipation based on context was also indexed by the P2 component. Specifically,

P2 amplitude increased with longer current durations, suggesting that it reflects hazard-based

expectancy: the probability that the interval offset will occur, given that is has not yet occurred

(Nobre, Correa, & Coull, 2007). This in line with previous studies showing that longer ISIs increase

P2 amplitude (e.g., Pereira et al., 2014; Röder et al., 2000). Importantly, however, P2 amplitude

decreased with longer previous durations, showing that the expectations are updated to the current

temporal context, even on a trial-by-trial basis. These results complement previous studies showing

that temporal expectancy modulates ERP amplitude (e.g., Kononowicz & van Rijn, 2014; Li et al.,

2017; Todorovic & de Lange, 2012; Todorovic, van Ede, Maris, & de Lange, 2011; Wacongne et al.,

2011). Interestingly, P2 amplitude at perception phase offset predicted interval reproductions, and

participants' behavioral context effect correlated with their context-based P2 effect. The lack of an

equivalent CNV-effect highlights the predictive quality of the P2 (Kononowicz & van Rijn, 2014;

Kruijne et al., 2021), and indicates that the neural state at the end of the perception phase sets the

speed of cortical dynamics during reproduction (Sohn et al., 2019). Global context additionally

influenced beta power, such that beta power was higher in the long compared to the short context, in

line with effects of beta power in single trial analyses (Kononowicz & van Rijn, 2015). Although beta

power has been proposed to reflect motor inhibition (Alegre et al., 2004; Hwang, Ghuman, Manoach,

Jones, & Luna, 2014; Kononowicz & van Rijn, 2015; Kühn et al., 2004), and most studies on the link

between beta power and timing have a strong motor component, our results suggest that synchronized

beta oscillations also play a role during interval perception after which no immediate motor response

is required. This finding complements recent studies showing that the accuracy and precision of time

estimates depend on beta (Wiener et al., 2018) and alpha-beta coupling (Kononowicz, Sander, van

Rijn, & Van Wassenhove, 2020). Additionally, the current global context effect on beta is in line with

Wiener et al.'s finding that longer previous durations increased beta power in the current trial. It has

to be noted, however, that we found no evidence for similar sequential effects on beta.

Besides the auditory stimuli which participants had to time, the current paradigm also

consisted of visual stimuli that indicated the phase of the trial (i.e., perception or reproduction). The

general overestimation we found in the behavioral results might potentially be explained by the

integration of these visual stimuli in temporal estimation (Shi & Burr, 2016). Future studies might

look further into potential modality differences in contextual calibration and their neural

underpinnings (Rhodes, Seth, & Roseboom, 2018; Roach et al., 2017; Zimmermann & Cicchini,

2020). Furthermore, we found no significant decoding corresponding to the windows of CNV

differences. This can be explained by the specific decoding method we employed, which focused on

transient dynamics, filtering out the stable CNV activity by baselining within a moving window. In

addition, decoding might be especially sensitive to stimulus onset and offset, with accuracy peaking

shortly afterwards and slowly dropping as the neural synchronization declines (e.g., Wolff et al.,

2017, 2020).

A comparison to Wiener and Thompson (2015), who found a larger CNV amplitude for

longer prior durations, suggests that contextual ERP effects might be dependent on the specific

experimental paradigm. In contrast to our reproduction experiment, their bisection task requires an

active decision during perception, and the CNV has been shown to reflect this decision process by

deflecting or plateauing after the standard interval in memory has been reached (Macar & Vidal,

2004; Ng et al., 2011; Pfeuty, Ragot, & Pouthas, 2003). A similar explanation could account for the

different nature of our offset P2 effect compared to Kononowicz and van Rijn (2014), who found a V-

shaped P2 amplitude attenuation in a temporal comparison task (but see Kruijne et al., 2021). This

pattern reflects active comparison to the standard interval, which is not applicable to the current

reproduction paradigm. In addition, the P2 measured in the current study shows similarities to the

positive offset peak named the late positive component of timing (LPCt) (Gontier et al., 2009; Paul et

al., 2011; Wiener & Thompson, 2015), although it has been argued that the P2 reflects perceptual

predictive processes while the LPCt indexes decision making (Kononowicz, van Rijn, & Meck, 2016).

The extent to which these components indeed reflect similar processes is still an open question, and

their occurrence seems to depend on the specific nature of the task. Future studies might directly

compare these neural differences in paradigms involving decision, motor or only perceptual timing

requirements.

454   In conclusion, our results show that previous durations actively influence flexible neural

455   dynamics during temporal encoding. These findings indicate that previous experiences in memory

456   create expectations that in turn calibrate our perception of the environment. The adaptive influence of

457   prior knowledge on perception could represent a more general Bayesian mechanism of magnitude

458   estimation (Petzschner, Glasauer, & Stephan, 2015), falsifying a class of models that assume discrete,

459   post-perceptual stages in which previous experiences exert their influence.

460   **Acknowledgements**

This research has been partially supported by the EU Horizon 2020 FET Proactive grant

TIMESTORM - Mind and Time: Investigation of the Temporal Traits of Human-Machine

Convergence (Grant number 641100) and by the research programme Interval Timing in the Real

World financed by the Netherlands Organisation for Scientific Research (NWO, Grant number 453-

16-005, awarded to Hedderik van Rijn). The funding agencies had no involvement in the design of the

study, the analysis of the data, writing of the report, or in the decision to submit the article for

publication. We thank Sarah Maaß for fruitful discussions and programming the experiment, Ronja

Eike for her help in data collection and preprocessing, Emil Uffelmann for his help in data collection,

and Michael Wolff and Güven Kandemir for sharing their decoding knowledge with us.

References

Acerbi, L., Wolpert, D. M., & Vijayakumar, S. (2012). Internal Representations of Temporal Statistics and Feedback Calibrate Motor-Sensory Interval Timing. *PLoS Computational Biology*, *8*(11). https://doi.org/10.1371/journal.pcbi.1002771

Alegre, M., De Gurtubay, I. G., Labarga, A., Iriarte, J., Malanda, A., & Artieda, J. (2004). Alpha and beta oscillatory activity during a sequence of two movements. *Clinical Neurophysiology*, *115*(1), 124–130. https://doi.org/10.1016/S1388-2457(03)00311-0

Bates, D., Mächler, M., Bolker, B. M., & Walker, S. C. (2015). Fitting linear mixed-effects models using lme4. *Journal of Statistical Software*, *67*(1). https://doi.org/10.18637/jss.v067.i01

Boehm, U., Van Maanen, L., Forstmann, B., & van Rijn, H. (2014). Trial-by-trial fluctuations in CNV amplitude reflect anticipatory adjustment of response caution. *NeuroImage*, *96*, 95–105. https://doi.org/10.1016/j.neuroimage.2014.03.063

Brainard, D. H. (1997). The Psychophysics Toolbox. *Spatial Vision*, *10*(4), 433–436. https://doi.org/10.1163/156856897X00357

Casini, L., & Vidal, F. (2011). The SMAs: Neural substrate of the temporal accumulator? *Frontiers in Integrative Neuroscience*, *5*, 1–3. https://doi.org/10.3389/fnint.2011.00035

Cicchini, G. M., Arrighi, R., Cecchetti, L., Giusti, M., & Burr, D. C. (2012). Optimal encoding of interval timing in expert percussionists. *Journal of Neuroscience*, *32*(3), 1056–1060. https://doi.org/10.1523/JNEUROSCI.3411-11.2012

Cicchini, G. M., Benedetto, A., & Burr, D. C. (2020). Perceptual history propagates down to early levels of sensory analysis. *Current Biology*. https://doi.org/10.1016/j.cub.2020.12.004

Cicchini, G. M., Mikellidou, K., & Burr, D. (2017). Serial dependencies act directly on perception. *Journal of Vision*, *17*(14). https://doi.org/10.1167/17.14.6

Coull, J. T., Vidal, F., & Burle, B. (2016). When to act, or not to act: That's the SMA's question. *Current Opinion in Behavioral Sciences*, Vol. 8, pp. 14–21. https://doi.org/10.1016/j.cobeha.2016.01.003

De Maesschalck, R., Jouan-Rimbaud, D., & Massart, D. L. (2000). The Mahalanobis distance. *Chemometrics and Intelligent Laboratory Systems*, *50*(1), 1–18. https://doi.org/10.1016/S0169-7439(99)00047-7

Di Luca, M., & Rhodes, D. (2016). Optimal Perceived Timing: Integrating Sensory Information with Dynamically Updated Expectations. *Scientific Reports*, *6*, 1–15. https://doi.org/10.1038/srep28563

Dyjas, O., Bausenhart, K. M., & Ulrich, R. (2012). Trial-by-trial updating of an internal reference in discrimination tasks: Evidence from effects of stimulus order and trial sequence. *Attention, Perception, and Psychophysics*, *74*(8), 1819–1841. https://doi.org/10.3758/s13414-012-0362-4

Elbert, T. (1993). Slow Cortical Potentials Reflect the Regulation of Cortical Excitability. In *Slow Potential Changes in the Human Brain* (pp. 235–251). https://doi.org/10.1007/978-1-4899-1597-9_15

Gontier, E., Paul, I., Le Dantec, C., Pouthas, V., Jean-Marie, G., Bernard, C., … Rebaï, M. (2009). ERPs in Anterior and Posterior Regions Associated With Duration and Size Discriminations. *Neuropsychology*, *23*(5), 668–678. https://doi.org/10.1037/a0015757

Grootswagers, T., Wardle, S. G., & Carlson, T. A. (2017). Decoding dynamic brain patterns from evoked responses: A tutorial on multivariate pattern analysis applied to time series neuroimaging data. *Journal of Cognitive Neuroscience*, *29*(4), 677–697. https://doi.org/10.1162/jocn_a_01068

Gu, B. M., Jurkowski, A. J., Lake, J. I., Malapani, C., & Meck, W. H. (2015). Bayesian Models of

Interval Timing and Distortions in Temporal Memory as a Function of Parkinson's Disease and Dopamine-Related Error Processing. In *Time Distortions in Mind* (pp. 281–327). https://doi.org/10.1163/9789004230699_012

Haegens, S., Nácher, V., Hernández, A., Luna, R., Jensen, O., & Romo, R. (2011). Beta oscillations in the monkey sensorimotor network reflect somatosensory decision making. *Proceedings of the National Academy of Sciences of the United States of America*, *108*(26), 10708–10713. https://doi.org/10.1073/pnas.1107297108

Hallez, Q., Damsma, A., Rhodes, D., van Rijn, H., & Droit-Volet, S. (2019). The dynamic effect of context on interval timing in children and adults. *Acta Psychologica*, *192*, 87–93. https://doi.org/10.1016/j.actpsy.2018.10.004

Hwang, K., Ghuman, A. S., Manoach, D. S., Jones, S. R., & Luna, B. (2014). Cortical neurodynamics of inhibitory control. *Journal of Neuroscience*, *34*(29), 9551–9561. https://doi.org/10.1523/JNEUROSCI.4889-13.2014

Jazayeri, M., & Shadlen, M. N. (2010). Temporal context calibrates interval timing. *Nature Neuroscience*, *13*(8), 1020–1026. https://doi.org/10.1038/nn.2590

Jenkinson, N., & Brown, P. (2011). New insights into the relationship between dopamine, beta oscillations and motor function. *Trends in Neurosciences*, *34*(12), 611–618. https://doi.org/10.1016/j.tins.2011.09.003

Kleiner, M., Brainard, D. H., Pelli, D. G., Broussard, C., Wolf, T., & Niehorster, D. (2007). What's new in Psychtoolbox-3? *Perception*, *36*, S14. https://doi.org/10.1068/v070821

Kononowicz, T. W., Sander, T., Van Rijn, H., & Van Wassenhove, V. (2020). Precision timing with α–β oscillatory coupling: Stopwatch or motor control? *Journal of Cognitive Neuroscience*, *32*(9), 1624–1636. https://doi.org/10.1162/jocn_a_01570

Kononowicz, T. W., & van Rijn, H. (2014). Decoupling interval timing and climbing neural activity: A dissociation between CNV and N1P2 amplitudes. *Journal of Neuroscience*, *34*(8), 2931–2939. https://doi.org/10.1523/JNEUROSCI.2523-13.2014

Kononowicz, T. W., & van Rijn, H. (2015). Single trial beta oscillations index time estimation. *Neuropsychologia*, *75*, 381–389. https://doi.org/10.1016/j.neuropsychologia.2015.06.014

Kononowicz, T. W., van Rijn, H., & Meck, W. H. (2016). Timing and time perception: a critical review of neural timing signatures before, during, and after the To-Be-Timed Interval. In *Stevens Handbook of Experimental Psychology and Cognitive Neuroscience (4th ed.)*.

Kruijne, W., Olivers, C. N. L., & van Rijn, H. (2021). Neural repetition suppression modulates time perception: Evidence from electrophysiology and pupillometry. *BioRxiv*, 2020.07.31.230508. https://doi.org/10.1101/2020.07.31.230508

Kühn, A. A., Williams, D., Kupsch, A., Limousin, P., Hariz, M., Schneider, G. H., … Brown, P. (2004). Event-related beta desynchronization in human subthalamic nucleus correlates with motor performance. *Brain*, *127*(4), 735–746. https://doi.org/10.1093/brain/awh106

Ledoit, O., & Wolf, M. (2004). Honey, I shrunk the sample covariance matrix. *Journal of Portfolio Management*, *30*(4), 110–119. https://doi.org/10.3905/jpm.2004.110

Lemm, S., Blankertz, B., Dickhaus, T., & Müller, K. R. (2011). Introduction to machine learning for brain imaging. *NeuroImage*, *56*(2), 387–399. https://doi.org/10.1016/j.neuroimage.2010.11.004

Leuthold, H., Sommer, W., & Ulrich, R. (2004). Preparing for action: Inferences from CNV and LRP. *Journal of Psychophysiology*, *18*(2–3), 77–88. https://doi.org/10.1027/0269-8803.18.23.77

Li, B., Chen, Y., Xiao, L., Liu, P., & Huang, X. (2017). Duration adaptation modulates EEG correlates of subsequent temporal encoding. *NeuroImage*, *147*(2), 143–151. https://doi.org/10.1016/j.neuroimage.2016.12.015

Liesefeld, H. R. (2018). Estimating the Timing of Cognitive Operations With MEG/EEG Latency
Measures: A Primer, a Brief Tutorial, and an Implementation of Various Methods. *Frontiers in*
Neuroscience, *12*. https://doi.org/10.3389/fnins.2018.00765

Luck, S. J. (2005). An Introduction to Event-Related Potentials and Their Neural Origins. *An*
Introduction to the Event-Related Potential Technique.

Maaß, S. C., Riemer, M., Wolbers, T., & van Rijn, H. (2019). Timing deficiencies in amnestic Mild
Cognitive Impairment: Disentangling clock and memory processes. *Behavioural Brain*
Research, *373*, 112110. https://doi.org/10.1016/j.bbr.2019.112110

Maaß, S. C., Schlichting, N., & van Rijn, H. (2019). Eliciting contextual temporal calibration: The
effect of bottom-up and top-down information in reproduction tasks. *Acta Psychologica*, *199*,
102898. https://doi.org/10.1016/j.actpsy.2019.102898

Macar, F., & Besson, M. (1985). Contingent negative variation in processes of expectancy, motor
preparation and time estimation. *Biological Psychology*, *21*(4), 293–307.
https://doi.org/10.1016/0301-0511(85)90184-X

Macar, F., & Vidal, F. (2004). Event-related potentials as indices of time processing: A review.
Journal of Psychophysiology, Vol. 18, pp. 89–104. https://doi.org/10.1027/0269-8803.18.23.89

Macar, F., Vidal, F., & Casini, L. (1999). The supplementary motor area in motor and sensory timing:
Evidence from slow brain potential changes. *Experimental Brain Research*, *125*(3), 271–280.
https://doi.org/10.1007/s002210050683

Macar, F., & Vitton, N. (1982). An early resolution of contingent negative variation (CNV) in time
discrimination. *Electroencephalography and Clinical Neurophysiology*, *54*(4), 426–435.
https://doi.org/10.1016/0013-4694(82)90206-1

Maris, E., & Oostenveld, R. (2007). Nonparametric statistical testing of EEG- and MEG-data. *Journal*
of Neuroscience Methods, *164*(1), 177–190. https://doi.org/10.1016/j.jneumeth.2007.03.024

Mento, G. (2013). The passive CNV: Carving out the contribution of task-related processes to
expectancy. *Frontiers in Human Neuroscience*, *7*, 827.
https://doi.org/10.3389/fnhum.2013.00827

Miniussi, C., Wilding, E. L., Coull, J. T., & Nobre, A. C. (1999). Orienting attention in time.
Modulation of brain potentials. *Brain*, *122*(8), 1507–1518.
https://doi.org/10.1093/brain/122.8.1507

Müller-Gethmann, H., Ulrich, R., & Rinkenauer, G. (2003). Locus of the effect of temporal
preparation: Evidence from the lateralized readiness potential. *Psychophysiology*, *40*(4), 597–
611. https://doi.org/10.1111/1469-8986.00061

Ng, K. K., Tobin, S., & Penney, T. B. (2011). Temporal accumulation and decision processes in the
duration bisection task revealed by contingent negative variation. *Frontiers in Integrative*
Neuroscience, *5*, 77. https://doi.org/10.3389/fnint.2011.00077

Nobre, A. C., Correa, A., & Coull, J. (2007). The hazards of time. *Current Opinion in Neurobiology*,
17(4), 465–470. https://doi.org/10.1016/j.conb.2007.07.006

Oostenveld, R., Fries, P., Maris, E., & Schoffelen, J. M. (2011). FieldTrip: Open source software for
advanced analysis of MEG, EEG, and invasive electrophysiological data. *Computational*
Intelligence and Neuroscience, *2011*. https://doi.org/10.1155/2011/156869

Paul, I., Wearden, J., Bannier, D., Gontier, E., Le Dantec, C., & Rebaï, M. (2011). Making decisions
about time: Event-related potentials and judgements about the equality of durations. *Biological*
Psychology, *88*(1), 94–103. https://doi.org/10.1016/j.biopsycho.2011.06.013

Pereira, D. R., Cardoso, S., Ferreira-Santos, F., Fernandes, C., Cunha-Reis, C., Paiva, T. O., …
Marques-Teixeira, J. (2014). Effects of inter-stimulus interval (ISI) duration on the N1 and P2

components of the auditory event-related potential. *International Journal of Psychophysiology*, *94*(3), 311–318. https://doi.org/10.1016/j.ijpsycho.2014.09.012

Petzschner, F. H., Glasauer, S., & Stephan, K. E. (2015). A Bayesian perspective on magnitude estimation. *Trends in Cognitive Sciences*, *19*(5), 285–293. https://doi.org/10.1016/j.tics.2015.03.002

Pfeuty, M., Ragot, R., & Pouthas, V. (2003). When time is up: CNV time course differentiates the roles of the hemispheres in the discrimination of short tone durations. *Experimental Brain Research*, *151*(3), 372–379. https://doi.org/10.1007/s00221-003-1505-6

Pfeuty, M., Ragot, R., & Pouthas, V. (2005). Relationship between CNV and timing of an upcoming event. *Neuroscience Letters*, *382*(1–2), 106–111. https://doi.org/10.1016/j.neulet.2005.02.067

R Core Development Team. (2013). A language and environment for statistical computing. *R Foundation for Statistical Computing*, Vol. 1. Retrieved from http://www.r-project.org/

Remington, E. D., Egger, S. W., Narain, D., Wang, J., & Jazayeri, M. (2018). A Dynamical Systems Perspective on Flexible Motor Timing. *Trends in Cognitive Sciences*, *22*(10), 938–952. https://doi.org/10.1016/j.tics.2018.07.010

Remington, E. D., Narain, D., Hosseini, E. A., & Jazayeri, M. (2018). Flexible Sensorimotor Computations through Rapid Reconfiguration of Cortical Dynamics. *Neuron*, *98*(5), 1005-1019.e5. https://doi.org/10.1016/j.neuron.2018.05.020

Rhodes, D., Seth, A. K., & Roseboom, W. (2018). Multiple Duration Priors Within and Across the Senses. *BioRxiv*, 467027. https://doi.org/10.1101/467027

Roach, N. W., McGraw, P. V., Whitaker, D. J., & Heron, J. (2017). Generalization of prior information for rapid Bayesian time estimation. *Proceedings of the National Academy of Sciences of the United States of America*, *114*(2), 412–417. https://doi.org/10.1073/pnas.1610706114

Röder, B., Rösler, F., & Neville, H. J. (2000). Event-related potentials during auditory language processing in congenitally blind and sighted people. *Neuropsychologia*, *38*(11), 1482–1502. https://doi.org/10.1016/S0028-3932(00)00057-9

Scheibe, C., Schubert, R., Sommer, W., & Heekeren, H. R. (2009). Electrophysiological evidence for the effect of prior probability on response preparation. *Psychophysiology*, *46*(4), 758–770. https://doi.org/10.1111/j.1469-8986.2009.00825.x

Schlichting, N., Damsma, A., Aksoy, E. E., Wächter, M., Asfour, T., & van Rijn, H. (2018). Temporal Context Influences the Perceived Duration of Everyday Actions: Assessing the Ecological Validity of Lab-Based Timing Phenomena. *Journal of Cognition*, *2*(1). https://doi.org/10.5334/joc.4

Shi, Z., & Burr, D. (2016). Predictive coding of multisensory timing. *Current Opinion in Behavioral Sciences*, *8*, 200–206. https://doi.org/10.1016/j.cobeha.2016.02.014

Shi, Z., Church, R. M., & Meck, W. H. (2013). Bayesian optimization of time perception. *Trends in Cognitive Sciences*, *17*(11), 556–564. https://doi.org/10.1016/j.tics.2013.09.009

Simen, P., Balci, F., deSouza, L., Cohen, J. D., & Holmes, P. (2011). A model of interval timing by neural integration. *Journal of Neuroscience*, *31*(25), 9238–9253. https://doi.org/10.1523/JNEUROSCI.3121-10.2011

Sohn, H., Narain, D., Meirhaeghe, N., & Jazayeri, M. (2019). Bayesian Computation through Cortical Latent Dynamics. *Neuron*, *103*(5), 934-947.e5. https://doi.org/10.1016/j.neuron.2019.06.012

St. John-Saaltink, E., Kok, P., Lau, H. C., & De Lange, F. P. (2016). Serial dependence in perceptual decisions is reflected in activity patterns in primary visual cortex. *Journal of Neuroscience*, *36*(23), 6186–6192. https://doi.org/10.1523/JNEUROSCI.4390-15.2016

Taatgen, N. A., & van Rijn, H. (2011). Traces of times past: Representations of temporal intervals in
memory. *Memory and Cognition*, *39*(8), 1546–1560. https://doi.org/10.3758/s13421-011-0113-0

Tanner, D., Morgan-Short, K., & Luck, S. J. (2015). How inappropriate high-pass filters can produce
artifactual effects and incorrect conclusions in ERP studies of language and cognition.
Psychophysiology, *52*(8), 997–1009. https://doi.org/10.1111/psyp.12437

Todorovic, A., & de Lange, F. P. (2012). Repetition suppression and expectation suppression are
dissociable in time in early auditory evoked fields. *Journal of Neuroscience*, *32*(39), 13389–
13395. https://doi.org/10.1523/JNEUROSCI.2227-12.2012

Todorovic, A., van Ede, F., Maris, E., & de Lange, F. P. (2011). Prior expectation mediates neural
adaptation to repeated sounds in the auditory cortex: An MEG study. *Journal of Neuroscience*,
31(25), 9118–9123. https://doi.org/10.1523/JNEUROSCI.1425-11.2011

Trillenberg, P., Verleger, R., Wascher, E., Wauschkuhn, B., & Wessel, K. (2000). CNV and temporal
uncertainty with "ageing" and "non-ageing" S1-S2 intervals. *Clinical Neurophysiology*, *111*(7),
1216–1226. https://doi.org/10.1016/S1388-2457(00)00274-1

Van der Lubbe, R. H. J., Los, S. A., Jaśkowski, P., & Verleger, R. (2004). Being prepared on time: On
the importance of the previous foreperiod to current preparation, as reflected in speed, force and
preparation-related brain potentials. *Acta Psychologica*, *116*(3), 245–262.
https://doi.org/10.1016/j.actpsy.2004.03.003

Wacongne, C., Labyt, E., Van Wassenhove, V., Bekinschtein, T., Naccache, L., & Dehaene, S.
(2011). Evidence for a hierarchy of predictions and prediction errors in human cortex.
Proceedings of the National Academy of Sciences of the United States of America, *108*(51),
20754–20759. https://doi.org/10.1073/pnas.1117807108

Wiener, M., Parikh, A., Krakow, A., & Coslett, H. B. (2018). An intrinsic role of beta oscillations in
memory for time estimation. *Scientific Reports*, *8*(1), 1–17. https://doi.org/10.1038/s41598-018-
26385-6

Wiener, M., & Thompson, J. C. (2015). Repetition enhancement and memory effects for duration.
NeuroImage, *113*, 268–278. https://doi.org/10.1016/j.neuroimage.2015.03.054

Wiener, M., Thompson, J. C., & Branch Coslett, H. (2014). Continuous carryover of temporal context
dissociates response bias from perceptual influence for duration. *PLoS ONE*, *9*(6).
https://doi.org/10.1371/journal.pone.0100803

Wolff, M. J., Jochim, J., Akyürek, E. G., & Stokes, M. G. (2017). Dynamic hidden states underlying
working-memory-guided behavior. *Nature Neuroscience*, *20*(6), 864–871.
https://doi.org/10.1038/nn.4546

Wolff, M. J., Kandemir, G., Stokes, M. G., & Akyürek, E. G. (2020). Unimodal and Bimodal Access
to Sensory Working Memories by Auditory and Visual Impulses. *The Journal of Neuroscience :
The Official Journal of the Society for Neuroscience*, *40*(3), 671–681.
https://doi.org/10.1523/JNEUROSCI.1194-19.2019

Zimmermann, E., & Cicchini, G. M. (2020). Temporal Context affects interval timing at the
perceptual level. *Scientific Reports*. https://doi.org/10.1038/s41598-020-65609-6

693