

1 Infrared absorptions as indicators for
2 *Pseudomonas aeruginosa* and
3 *Acinetobacter baumannii*

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19 **Abstract**

20 There is clinical demand for simple and contact-free diagnosis techniques in medical practice. This
21 study shows that the infrared absorptions of volatile metabolites can be used to distinguish between
22 the air around *Pseudomonas aeruginosa*, *Acinetobacter baumannii*, other bacteria, and normal room
23 air. Gas samples were collected from the air surrounding single and mixed laboratory cultures, and
24 preliminary data on human breath samples are also presented. The infrared spectra of a variety of
25 gasses are measured with a high resolution of 0.5 cm^{-1} to obtain information about the wavenumber
26 position of the key bands. Hence, it is not necessary to specify the molecular species of biomarkers.
27 This work also shows that discrimination rates can be improved by observing additional infrared
28 absorptions caused by different characteristic volatile molecules. The significance of this work is that
29 the specific wavenumber positions of the key bands that allow the application of infrared lasers are
30 provided. As a result, it is considered that *Pseudomonas aeruginosa* and *Acinetobacter baumannii* can
31 be monitored more sensitively and easily. With further research and development, this simple
32 approach could be used in future applications to identify infections in healthcare settings.

33 **Introduction**

34 Biomarkers are characteristic molecules produced by biological processes. The biomarkers found
35 in various gas samples have been examined by using gas chromatography–mass spectrometry (GCMS),
36 and they are of interest for non-invasive diagnosis and healthcare applications [1–5]. In addition,

37 representative small molecules such as CO, CO₂, NO, and NO₂ have been the target of high-sensitivity
38 infrared laser spectroscopy measurements [6–9]. Clinical applications of these techniques have been
39 proposed [10–12].

40 To apply an infrared laser, it is necessary to adjust the oscillation wavenumber (the reciprocal of
41 the wavelength) to a specific value. A molecule produces many peaks, but the wavenumber indicates
42 the position of one strong peak on the horizontal axis of the infrared spectrum. Infrared lasers can be
43 used to detect changes in the concentration (partial pressure) of some target volatile biomarkers. In
44 particular, it has been shown that changes in the concentration of ethane [13] and ethanol [14] can be
45 detected with ultra-high sensitivity, in addition to the molecules CO, CO₂, NO, and NO₂.

46 High resolution infrared spectra can be obtained for a wide variety of gas samples. By analyzing
47 the infrared absorption peaks it is possible to identify the key band, the infrared absorption peak that
48 serves as the target index of a biomarker. There are two criteria for defining a key band. First, it must
49 appear in a “window” region where there are no unrelated strong peaks; this means the intensity of the
50 key band can be observed clearly. Second, the peak position of the wavenumber must be accurately
51 determined in a range close to the linewidth of the infrared laser.

52 The intensity and wavenumber position of the key band correspond to quantitative information
53 about the concentration (partial pressure) of key volatile metabolites (VMs) or volatile organic
54 compounds (VOCs). This information is the index equivalent to surveillance markers and can be used

55 to distinguish between bacterial species using the surrounding air.

56 In recent years, several reports [15–19] have classified bacteria based on infrared spectra measured
57 using Fourier-transform infrared (FTIR) spectroscopy. In these studies, samples were prepared by
58 treating cultured bacteria, and the analysis target was the bacteria itself, not the VMs released from
59 the bacteria. The infrared spectra were measured with a general resolution of 4 cm^{-1} by directly
60 irradiating bacteria with infrared light and transmitting or reflecting the light.

61 In this study, infrared spectra have been recorded for a wide variety of gas samples including gases
62 obtained near eight types of bacteria and reference samples of indoor air. Each of these gas samples
63 contains a wide variety of molecules, and each molecule (except for homonuclear diatomic molecules
64 such as O_2 and N_2) produces many infrared absorption peaks. An infrared spectrum for one gas sample
65 may include thousands of peaks in the range of $550\text{--}7000\text{ cm}^{-1}$. By analyzing the accumulation of the
66 infrared spectra, the wavenumber positions of the key bands (the characteristic infrared absorption
67 peaks) can be found. Therefore, the oscillation frequency (wavenumber) of the infrared laser can be
68 fine-tuned in a limited area, which makes it possible to detect bacteria with high sensitivity without
69 identifying the molecular species as the target index markers.

70 The characteristic molecules released into the atmosphere by some types of bacteria have also been
71 investigated using GCMS [20]. In particular, methyl thiocyanate and benzonitrile have been identified
72 as characteristic VOCs emitted by *Pseudomonas aeruginosa*. These molecules give strong infrared

73 absorption peaks in the region of 2000–2300 cm^{-1} . However, specifying the molecular structure of the
74 key VOC does not automatically mean it can be found because the key band must appear in the
75 “window” region so that the intensity can be read. The condition is confirmed only by comparison
76 with many infrared spectra of other gas samples.

77 The next condition is whether the accuracy of the key-band position is in a range that facilitates the
78 application of an infrared laser. Experimental results for a pure substance and the theoretical
79 calculations for a molecule, such as normal vibration analysis for the most stable structure, may be
80 used to predict candidates for the key bands. However, gas samples contain a mixture of substances
81 including H_2O , CO_2 , and other atmospheric components, which could affect the key-band position by
82 binding to the key molecule. Furthermore, the infrared spectra may potentially reflect molecular
83 aggregates, clusters, and small particles suspended in the atmosphere, which have a different structure
84 than that suggested by the GCMS. A key molecule does not always give the key bands at the same
85 position, intensity, and width as the prediction.

86 This study aims to identify the key bands that characterize the air around *Pseudomonas aeruginosa*
87 and *Acinetobacter baumannii*. These are typical drug-resistant bacteria that are associated with
88 nosocomial infections, so there is urgent need for simple and contact-free detection techniques that
89 can be used in medical practice. The wavenumber positions of the key bands can be used to
90 discriminate between gas samples without specifying the molecular species of the biomarkers.

91 Specifically, the wavenumber position of the key bands for VOCs or VMs emitted by the bacteria are
92 recorded at a high resolution of 0.5 cm^{-1} , which makes it possible to determine the type of bacteria
93 without contact. Furthermore, this work aims to demonstrate that the high intensity infrared absorption
94 peak that appears at a specific wavenumber position can be used as an indicator for nearby bacterial
95 growth, even if the molecular structure of the characteristic VOC(s) is not specified.

96 The positions of the key bands are found from the experimental results (the accumulation of infrared
97 spectra in the region of $550\text{--}7000\text{ cm}^{-1}$) for various mixed substances, as a result of the search and
98 selection. Therefore, the key substance is not limited to a single molecule in the most stable structure.
99 This differs from the previous studies because any suspended substances shown by the infrared
100 absorption peaks are covered.

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102 **Methods**

103 **Preparation of gas samples**

104 Gas samples were obtained from the air surrounding cultured bacteria. The gases were aspirated
105 into gas bags (smart bag PA, smart bag 2F, Tedlar bag or ANALYTIC-BARRIER bag, GL Sciences)
106 by the indirect sampling method using a dry pump. The gas bag was equipped with a standard sleeve
107 (6-7 mm O.D.) connected to a silicone tube within 1 m. The other end of the silicone tube was placed
108 within 5 cm of the object. Eight types of bacteria, including standard strains and hospital isolates, were

109 cultured in sheep's blood agar at 37 °C for 30 to 40 h. The details are summarized in Table 1. *M1*, *M2*,
110 *M3*, and *M4* indicate mixed gas samples obtained from plural types of bacteria cultured in a nutrient
111 agar at 37 °C. For comparison, normal room air, human breath, and air from the vicinity of the culture
112 medium alone were also obtained and measured. The human breath was blown into a polyethylene
113 zipper bag.

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Table 1. Details of the gas samples.

Air around bacteria	Genus species	ID	Strain/Origin	Number of samples	Total number of measurements	Incubation time (h)	
Standard strains	<i>Escherichia coli</i>	<i>Ec</i>	type strain (NBRC 3972)	2	8 (1+7)	32	
	<i>Staphylococcus aureus</i>	<i>Sa</i>	type strain (NBRC 13276)	2	8 (4+4)	39	
	<i>Pseudomonas aeruginosa</i>	<i>Pa1</i>	type strain (NBRC113275)	2	11 (5+6)	38.5	
	plural culture plates in a chamber for the mixed gas collection	<i>M1</i>	Ec+Sa		2	19 (7+12)	38*
		<i>M2</i>	Ec+Pa1		2	17 (3+14)	38*
		<i>M3</i>	Sa+Pa1		2	11 (3+8)	38*
		<i>M4</i>	Ec+Sa+Pa1		2	12 (5+7)	38*
Hospital isolates	<i>Pseudomonas aeruginosa</i>	<i>Pa2</i>	hospital environment 1	2	10 (5+5)	39	
		<i>Pa3</i>	hospital environment 2	2	10 (5+5)	39	
	<i>Acinetobacter baumannii</i>	<i>Ab1</i>	clinical isolate 1	2	11 (5+6)	38.5	
		<i>Ab2</i>	clinical isolate 2	2	10 (5+5)	38	
		<i>Ab3</i>	clinical isolate 3	2	10 (5+5)	38	
		<i>Ab4</i>	clinical isolate 4	2	11 (5+6)	39	
		<i>Ab5</i>	clinical isolate 5	2	11 (5+6)	39	
	<i>Enterobacter aerogenes</i>	<i>Ena</i>	clinical isolate	2	10 (4+6)	37.5	
	<i>Enterobacter cloacae</i>	<i>Enc</i>	clinical isolate	2	8 (1+7)	39	
	<i>Klebsiella pneumoniae</i>	<i>Kp</i>	clinical isolate	2	8 (1+7)	32	
	<i>Streptococcus pneumoniae</i>	<i>Sp1</i>	clinical isolate 1	2	10 (4+6)	37.5	
<i>Sp2</i>		clinical isolate 2	2	8 (4+4)	37.5		

* means a nutrient agar for the culture medium, the others are sheep blood agar.

Reference samples	air around the culture medium without bacterial breeding	blood agar	2	8(4+4)
	room air	nutrient agar	3	8(2+3+3)
	human breath	taken from 5 places		146
		taken from 3 health people		136

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131 **Measurements**

132 The gas in each bag was introduced into a gas cell (light path length 10 m) installed in an FTIR
133 spectrometer (Bruker VERTEX 70). Overall, 365 infrared (IR) spectra for the various gas samples in
134 Table 1 were measured in the range of 550–7500 cm^{-1} at atmospheric pressure with a resolution of 0.5
135 cm^{-1} .

136 **Data analysis**

137 Microsoft EXCEL was used for data processing and analysis. The details of the infrared absorption
138 peaks that appeared in the IR spectra were obtained and the peak intensities were measured and
139 compared. The peak intensity was calculated by subtracting the absorbance at the base point from that
140 at the absorption peak. Peak and base pairs were found around the peak positions where the target
141 group showed strong absorption. The mean and variance of the absorption intensity for the reference
142 group were compared with the target group. Peak and base pairs with high discrimination rates were
143 extracted for each, pair and high discrimination rates were achieved for *P. aeruginosa* and *A.*
144 *baumannii*.

145 **Ethics statement**

146 This study was approved by the research ethics committee of Showa University School of Medicine

147 (Approval No. 371 and 2510).

148 **Results and discussion**

149 ***Pseudomonas aeruginosa (Pa)***

150 Fig 1 shows the IR spectra at approximately 2213 cm⁻¹ for the air surrounding the eight types of
151 cultured bacteria and the normal room air. These nine spectra are offset and aligned. The vertical axis
152 indicates absorbance and the absorption peak appears in the upward direction. In this region of the IR
153 spectra, a strong peak can be observed at 2213.2 cm⁻¹, which is characteristic of *Pa*.

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155 **Fig 1. IR spectra at approximately 2213 cm⁻¹ for the air surrounding 8 types of bacteria and**
156 **room air.** The 9 spectra are offset and aligned in the following order from the top: *Pseudomonas*
157 *aeruginosa (Pa)*, *Klebsiella pneumoniae (Kp)*, *Escherichia coli (Ec)*, *Staphylococcus aureus (Sa)*,
158 *Enterobacter cloacae (Enc)*, *Enterobacter aerogenes (Ena)*, *Acinetobacter baumannii (Ab)*,
159 *Streptococcus pneumoniae (Pa)*, and room air.

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161 As shown by the two dotted lines in Fig 1, two positions in the wavenumber (horizontal axis) were
162 fixed to determine the relative intensity of the absorption peak (P) at 2213.2 cm⁻¹ (P at 2213.2)
163 compared to the value in absorbance of the base point (B) at 2213.7 cm⁻¹ (B at 2213.7). As indicated
164 by the two-way arrow in Fig 1, the difference was calculated by subtracting the absorption value at

165 the base point from that at the peak. This value was used as the intensity of the absorption peak at
166 2213.2 cm^{-1} assigned to the VM from *Pa*. In all of the spectra, the two fixed positions for the assumed
167 peak and base do not actually correspond to the wavenumbers at the local maximum and minimum,
168 respectively.

169 The absorption peaks at 2213.2 cm^{-1} and 778.4 cm^{-1} were taken as the index of *Pa*. The absorption
170 intensity of the peak at 778.4 cm^{-1} (P at 778.4) is the difference from the value for the base point at
171 778.6 cm^{-1} (B at 778.6).

172 Fig 2 shows the results for discrimination of *Pa* using two intensities as the *Pa* indexes. The
173 subtracted value, P at 778.4 - B at 778.6, is shown on the horizontal (x) axis, and that of P at 2213.2 -
174 B at 2213.7 is shown on the vertical (y) axis. The gas samples that included VMs from *Pa* (filled grey
175 squares ■) are grouped in the upper right region, which is delimited by two dotted lines ($x > 0$ and y
176 > 0.003). All of the other cases are distinguished. The 365 points in Fig 2 correspond to the values
177 obtained for the 365 spectra from the various gas samples shown in Table 1. Open circles ○ indicate
178 the values obtained from human breath samples. The infrared spectra of human breath were measured
179 under the same conditions as the air samples for cultured bacteria and they have been stored for
180 analysis. The results will be published in later works.

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182 **Fig 2. Discrimination of *Pseudomonas aeruginosa* (*Pa*) with two indexes, P at 778.4 - B at 778.6**

183 **and P at 2213.2 - B at 2213.7, shown on the horizontal (x) and vertical (y) axes, respectively.**

184 Grey squares ■, the values obtained from the gas samples that included VMs from *Pa*; open squares

185 □, the other 7 types of bacteria; black triangles ▲, air from the vicinity of the culture medium alone;

186 open triangles △, the normal room air; and open circles ○, human breath. *M2*, *M3*, and *M4* indicate

187 the data from the mixed gas samples that included VMs from *Pa* and the other type(s) of bacteria, as

188 shown in Table 1.

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190 The values on the *x* and *y* axes reflect the infrared absorption peaks of the VMs specific to *Pa*.

191 According to Lambert-Beer's law, the infrared absorption intensity indicated by absorbance is

192 proportional to the concentration or partial pressure. The gas samples contain multiple unknown

193 chemical species and the absorption peaks from the different components could overlap in the infrared

194 spectrum. In this case, the absorbance intensity would not show a simple proportional relationship.

195 The main VM(s) on the *x* axis is (are) different from that (those) on the *y* axis, because the points in

196 Fig 2 do not show a strong linear relationship. However, Fig 2 shows that *Pa* can be clearly detected

197 by infrared light with specific wavenumbers passing through the surrounding air.

198 GCMS has been used to show that methyl thiocyanate and benzonitrile are characteristic VMs of

199 *Pa* [20]. These VMs produce strong infrared absorption peaks in the region of 2000–2300 cm⁻¹, where

200 one *Pa* index (P at 2213.2 - B at 2213.7) appears. Typical VMs, CO, and N₂O also give strong infrared

201 absorption peaks in the same region. However, this study does not exclude other VMs that may
202 produce the index peak, because FTIR does not require the ionization of VMs and can provide
203 information about unstable VMs, unlike GCMS.

204 *Acinetobacter baumannii* (*Ab*)

205 Fig 3 shows the result for discrimination of *Ab* using two intensities as the *Ab* indexes. One is the
206 peak intensity at 1215.0 cm⁻¹ which the subtracted value P at 1215.0 - B at 1214.5, as shown on the
207 horizontal (x) axis, and the other is P at 2982.3 - B at 2982.9, as shown on the vertical (y) axis. The
208 points represent gas samples including the VMs from *Ab* (filled grey square mark ■) that are shown
209 in the region between the two dotted lines ($y > 3.76x$ and $y < 9.65x$). Almost all the other cases are
210 distinguished.

211 The *Ab* index, the intensity of the absorption peak at 2982.3 cm⁻¹ is in the CH stretching vibration
212 region; this indicates that the causative VM molecule contains a hydrocarbon structure characteristic
213 of *Ab*. The other *Ab* index observed at 1215.0 cm⁻¹ is derived from another VM and the ratio of these
214 VMs is specific to *Ab*, as shown in Fig 3.

215

216 **Fig 3. Discrimination of *Acinetobacter baumannii* (*Ab*) with two *Ab* indexes, P at 1215.0 - B at**
217 **1214.5 and P at 2982.3 - B at 2982.9, shown on the horizontal (x) and vertical (y) axes,**
218 **respectively.** Grey squares ■, the values obtained from the gas samples that included VMs from

219 *Acinetobacter baumannii* (*Ab*); black triangles ▲, air from the vicinity of the culture medium
220 alone; black diamonds ◆, *Escherichia coli* (*Ec*); open squares □, the other 6 types of bacteria
221 in Table 1 except *Ab* and *Ec*; open triangles △, the normal room air; and open circles ○, human
222 breath.

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224 In Fig 3, the *Ab* area ($y > 3.76x$ and $y < 9.65x$, a triangular zone between the two dotted lines)
225 overlaps with other plots in the lower left corner. This is due to the detection sensitivity and the
226 wavenumber resolution of the FTIR spectroscopy and it could be improved by adopting an infrared
227 laser system. The *Ab* area also overlaps with the areas for *Escherichia coli* (*Ec*, ◆ filled black diamond)
228 and the blood agar medium (▲ filled black triangle in the upper left), which causes the *Ab*
229 discrimination rate to deteriorate.

230 Two additional indices of *Ab* were found, as shown in Fig 4, indicating there was an infrared
231 absorption peak at 4768.7 cm^{-1} (P at 4768.7 - B at 4768.1) on the x axis and 5353.8 cm^{-1} (P at 5353.8
232 - B at 5354.4) on the y axis. The two dotted lines ($y = -188x$ and $y = 78x$) separate the points for *Ab*,
233 *Ec*, and culture medium only. By combining the information from Figs 3 and 4, the rate of *Ab*
234 discrimination can be increased.

235

236 **Fig 4. Discrimination between *Acinetobacter baumannii* (*Ab*), *Escherichia coli* (*Ec*), and the blood**

237 **agar medium only, with two additional indexes P at 4768.7 - B at 4768.1 and P at 5353.8 - B at**
238 **5354.4, shown on the horizontal (x) and vertical (y) axes, respectively.** Grey squares ■, the
239 values obtained from IR spectra for the gas samples including the VMs from *Acinetobacter*
240 *baumannii* (*Ab*); black triangles ▲, air from the vicinity of the culture medium alone; and black
241 diamonds ◆, *Escherichia coli* (*Ec*).

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243 In Fig 4, one of the dotted straight lines has a negative slope, and some plots are in the negative
244 region of the horizontal axis (x). Typically, the value of P at 4768.7 - B at 4768.1 is considered positive,
245 because the wavenumber positions at 4768.7 and 4768.1 are assumed to be at the peak (P) and bottom
246 (B), respectively. In fact, none of the gas samples gave the expected infrared spectra. Some gas
247 samples contain a VM that gives an infrared absorption peak where we assume the bottom. This is a
248 reason why not all discrimination lines are ideally based on Lambert-Beer's law.

249

250 **Application and data processing**

251 Infrared lasers can be applied to detect the key VMs of *Pa* and *Ab* using three steps:

252 (1) fine adjustments of the oscillation wavenumbers at the absorption peak (P) and base point (B);

253 (2) conversions of the outputs from the light receiving parts in the infrared laser system to values

254 comparable to the results in this report; and

255 (3) a discrimination program with consideration of the optical path length.

256 It is worth noting that the gas samples in this experiment were under atmospheric pressure. This
257 work assumes that the atmospheric pressure during any application is the same as at the experiment
258 site.

259 To replace the absorbance (A) obtained by FTIR spectroscopy with the intensity (I) obtained from
260 the infrared laser system, the wavenumber positions of P and B were reported as a pair. The
261 relationship between the absorbance (A) and transmittance (T) is

$$262 \quad A = -\log(T) = -\log(I_{\text{sample}}/I_{\text{blanc}}) \quad (1)$$

263 where I_{sample} and I_{blanc} are the raw values of intensity with and without a sample, respectively. In
264 addition,

$$265 \quad A_{\text{at P}} - A_{\text{at B}} = -\log(T_{\text{at P}}/T_{\text{at B}}) \\ 266 \quad = -\log((I_{\text{sample at P}}/I_{\text{blanc at P}}) / (I_{\text{sample at B}}/I_{\text{blanc at B}})) \quad (2)$$

267 where $A_{\text{at P}}$ and $A_{\text{at B}}$ are the absorption values at P and B, respectively.

268 Infrared lasers have a narrow linewidth and do not give the intensity other than a specific
269 wavenumber. In contrast, FTIR spectroscopy produces a continuous spectrum and the intensity of the
270 infrared light source changes slightly with the wavenumber. In the absence of absorption effects,
271 within a 1 cm^{-1} range, the intensity is assumed to be constant; that is, $I_{\text{blanc at P}} \approx I_{\text{blanc at B}}$. Therefore,
272 from (2) it is possible to obtain

273
$$A_{\text{at P}} - A_{\text{at B}} \approx -\log(I_{\text{at P}} / I_{\text{at B}}) \quad (3)$$

274 where $I_{\text{at P}}$ and $I_{\text{at B}}$ are the raw intensity values at P and B, respectively, which can be observed by
275 the infrared laser system.

276 The value of $A_{\text{at P}} - A_{\text{at B}}$ reflects to the partial pressure (concentration) of a key VM. Two sets of
277 $A_{\text{at P}}$ and $A_{\text{at B}}$ for two key VMs can provide information about their component ratios. An appropriate
278 combination of these sets can be used to show the characteristics of the gas sample more clearly.

279 The discriminant in Figs 2–4 is based on the measurements obtained using a gas cell with an optical
280 path length of 10 m. According to Lambert-Beer's law, the absorbance is proportional to the optical
281 path length under the same pressure. If the optical path length is L m, which is part of the discriminant,
282 then $y > 0.003$ shown in Fig 2 becomes $y > 0.003 \times L / 10$. In addition, $x > 0$ in Fig 2, $y = 9.65x$ and y
283 $= 3.76x$ in Fig 3, and $y = -188x$ and $y = 78x$ in Fig 4 are linear functions through the origin that are not
284 dependent on the optical length.

285 Since the absorption intensity is proportional to the optical path length, the longer the optical path
286 length, the better the sensitivity. For this reason, infrared laser systems have an advantage over other
287 methods for analyzing low-density gas samples. Most biogas samples are obtained non-invasively.
288 Further, infrared light generally has low energy and is non-destructive. Therefore, it would be realistic
289 to monitor the environment in an open-path space by passing infrared laser light in medical, clinical,
290 and general life settings. When optimizing the optical path according to the required sensitivity and

291 the size of the space to be examined, multiple reflections can be used to increase the optical path length
292 even in a small space, and to achieve high sensitivity.

293

294 **Conclusion**

295 This study demonstrated that *P. aeruginosa* and *A. baumannii* can be detected using infrared lights
296 with specific wavenumbers that pass through the surrounding air. The discrimination rates can be
297 improved by observing additional infrared absorptions caused by different key VMs. The results can
298 be used in the application of infrared lasers for continuous monitoring of *P. aeruginosa* and *A.*
299 *baumannii* with high sensitivity.

300 The next step involves fine-tuning of the oscillating wavenumber of the infrared laser around the
301 values reported in this study. The fine adjustment will be performed by finding a wavenumber position
302 with the best discrimination rate in consideration of the line width of the infrared laser. As the result,
303 comparisons with traditional methods will be possible.

304 Applications for human health care will require the accumulation of more detailed information in
305 the infrared spectrum for gas samples under more diverse conditions. We believe that information
306 related to human health, which is statistically significant and has a high discrimination rate, can be
307 extracted by enhancement of the database. At present, we are working with hospitals to accumulate
308 infrared spectra of biogas samples from patients.

309

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314

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316 **References**

- 317 [1] Amann A, Smith D. Volatile Biomarkers: Non-Invasive Diagnosis in Physiology and Medicine.
318 Science Direct, Elsevier; 2013.
- 319 [2] Jia Z, Patra A, Kutty VK, Venkatesan T. Critical Review of Volatile Organic Compound Analysis
320 in Breath and In Vitro Cell Culture for Detection of Lung Cancer. *Metabolites*. 2019; 9:52.
- 321 [3] Saalberg Y, Wolff M. VOC breath biomarkers in lung cancer. *Clinica Chimica Acta*. 2016; 459:5.
- 322 [4] Wilson AD. Advances in Electronic-Nose Technologies for the Detection of
323 Volatile Biomarker Metabolites in the Human Breath. *Metabolites*. 2015; 5:140.
324 DOI: 10.3390/metabo5010140.
- 325 [5] Sethi S, Nanda R, Chakraborty T. Clinical Application of Volatile Organic Compound Analysis
326 for Detecting Infectious Diseases. *Clin Microbiol Rev*. 2013; 26(3):462.
- 327 [6] Popp A, Müller F, Kühnemann F, Schiller S, von Basum G, Dahnke H, et al. Ultra-sensitive mid-
328 infrared cavity leak-out spectroscopy using a cw optical parametric oscillator. *Appl Phys B*. 2002;
329 75(6–7):751.
- 330 [7] Engel GS, Drisdell WS, Keutsch FN, Moyer EJ, Anderson JG. Ultrasensitive near-infrared
331 integrated cavity output spectroscopy technique for detection of CO at 1.57 μm : new sensitivity limits
332 for absorption measurements in passive optical cavities. *Appl Opt*. 2006; 45(36):9221.
- 333 [8] Shorter JH, Nelson DD, McManus JB, Zahniser MS, Sama S, Milton DK. Clinical study of

- 334 multiple breath biomarkers of asthma and COPD (NO, CO₂, CO and N₂O) by infrared laser
335 spectroscopy. *J Breath Res.* 2011; 5(3):037108.
- 336 [9] Mandon J, Högman M, Merkus PJFM, van Amsterdam J, Harren FJM, Cristescu SM. Exhaled
337 nitric oxide monitoring by quantum cascade laser: comparison with chemiluminescent and
338 electrochemical sensors. *J Biomed Opt.* 2012; 17(1):017003.
- 339 [10] Mürtz M, Halmer D, Horstjann M, Thelen S, Hering P. Ultra sensitive trace gas detection for
340 biomedical applications. *Spectrochim Acta A Mol Biomol Spectrosc.* 2006; 63(5)L:963. DOI:
341 10.1016/j.saa.2005.11.015.
- 342 [11] Kim S-S, Young C, Vidakovic B, Gabram-Mendola SGA, Bayer CW, Mizaikoff B. Potential and
343 Challenges for Mid-Infrared Sensors in Breath Diagnostics. *IEEE Sens.* 2010; 10(1):145. DOI:
344 10.1109/JSEN.2009.2033940.
- 345 [12] Henderson B, Khodabakhsh A, Metsälä M, Ventrillard I, Schmidt FM, Romanini D, et al. Laser
346 spectroscopy for breath analysis: towards clinical implementation. *Appl Phys B.* 2018; 124:161. DOI:
347 10.1007/s00340-018-7030-x.
- 348 [13] von Basum G, Dahnke H, Halmer D, Hering P, Mürtz M. Online recording of ethane traces in
349 human breath via infrared laser spectroscopy. *J Appl Physiol.* 2003; 95(6):2583. DOI:
350 10.1152/jappphysiol.00542.2003.
- 351 [14] Jones AW, Andersson L. Determination of ethanol in breath for legal purposes using a five-filter

- 352 infrared analyzer: studies on response to volatile interfering substances. J Breath Res. 2008;
353 2(2):026006. DOI: 10.1088/1752-7155/2/2/026006.
- 354 [15] Fischer G, Braun S, Thissen R, Dott W. FT-IR spectroscopy as a tool for rapid identification and
355 intra-species characterization of airborne filamentous fungi. J Microbiol Methods. 2006; 64:63.
- 356 [16] Taha M, Hassan M, Essa S, Tartor Y. Use of Fourier transform infrared spectroscopy (FTIR)
357 spectroscopy for rapid and accurate identification of Yeasts isolated from human and animals. Int J
358 Vet Sci Med. 2013; 1:15.
- 359 [17] Maity JP, Kar S, Lin C-M, Chen C-Y, Chang Y-F, Jean J-S, et al. Identification and discrimination
360 of bacteria using Fourier transform infrared spectroscopy. Spectrochim Acta A Mol Biomol Spectrosc.
361 2013; 116:478.
- 362 [18] Alvarez-Ordóñez A, Mouwen DJM, López M, Prieto M. Fourier transform infrared spectroscopy
363 as a tool to characterize molecular composition and stress response in foodborne pathogenic bacteria.
364 J Microbiol Methods. 2011; 84:369.
- 365 [19] Nagib S, Rau J, Sammra O, Laßmüller C, Schlez K, et al. Identification of *Trueperella pyogenes*
366 isolated from bovine mastitis by Fourier transform infrared spectroscopy. PLOS ONE. 2014; 9(8):
367 e104654. DOI:10.1371/journal.pone.0104654
- 368 [20] Bos LDJ, Sterk PJ, Schultz MJ. Volatile Metabolites of Pathogens: A Systematic Review.
369 PLOS Pathogens. 2013; 9(5):1.

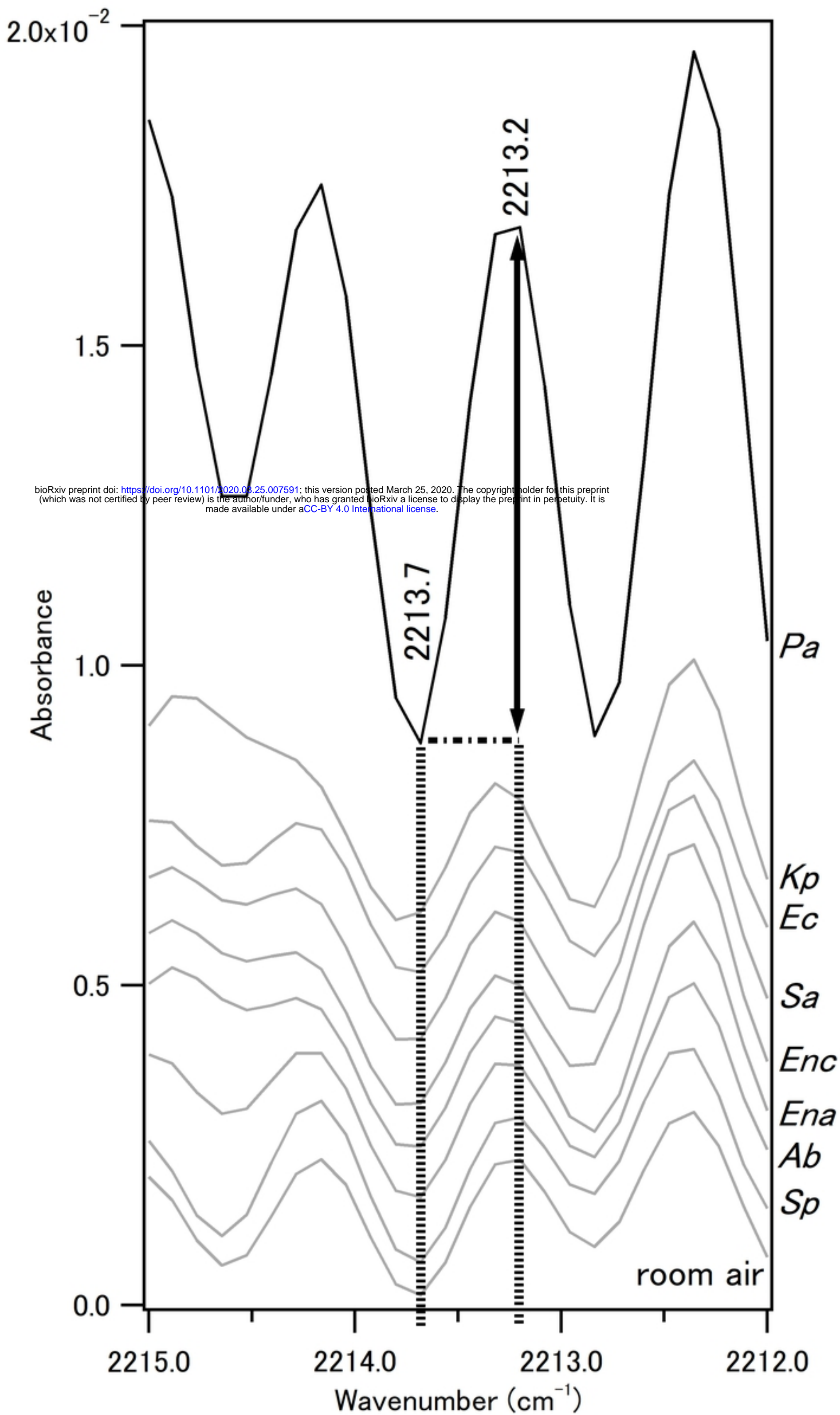


Figure 1

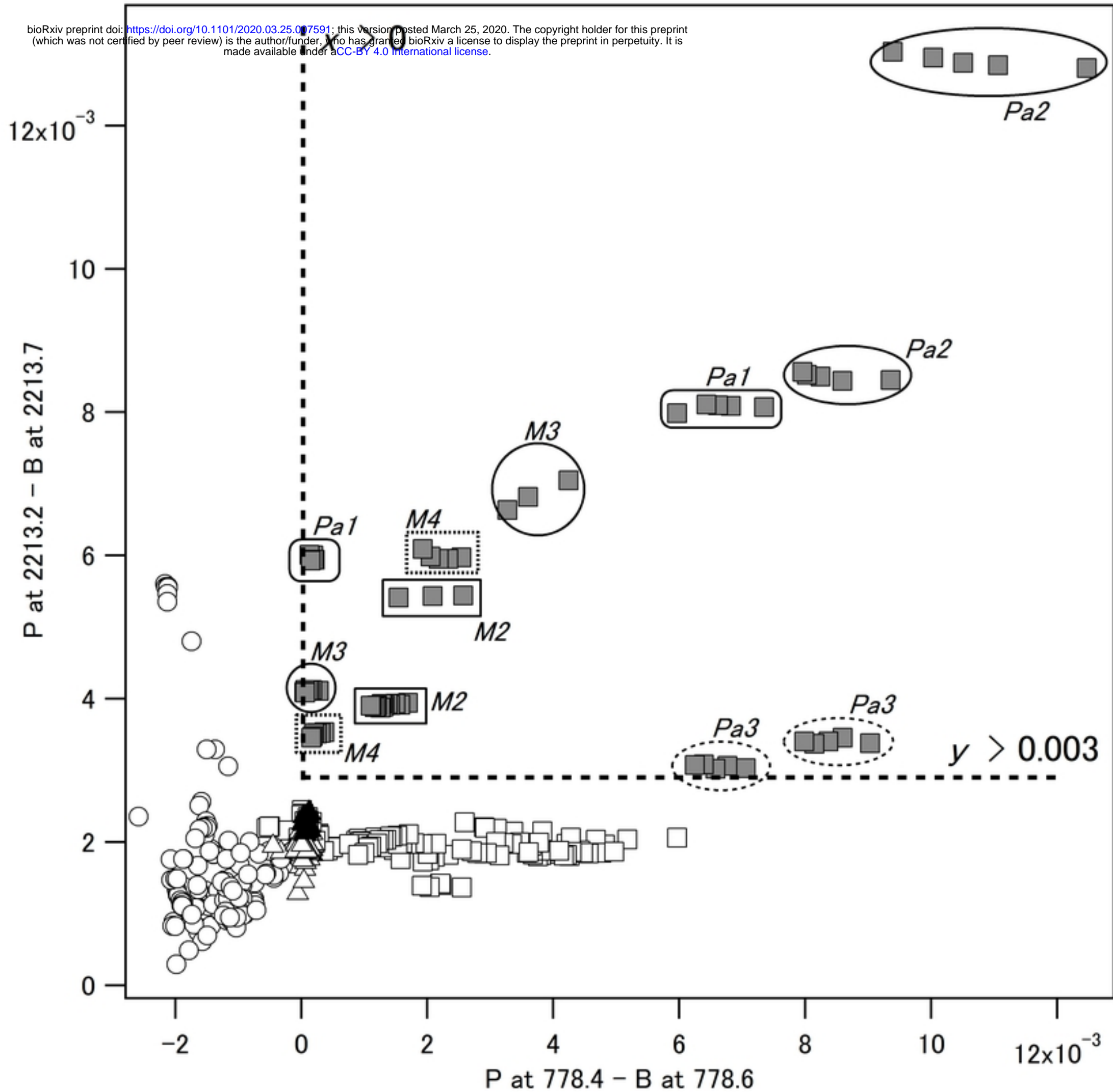


Figure 2

8×10^{-3}

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P at 2982.3 - B at 2982.9

P at 1215.0 - B at 1214.5

3.0×10^{-3}

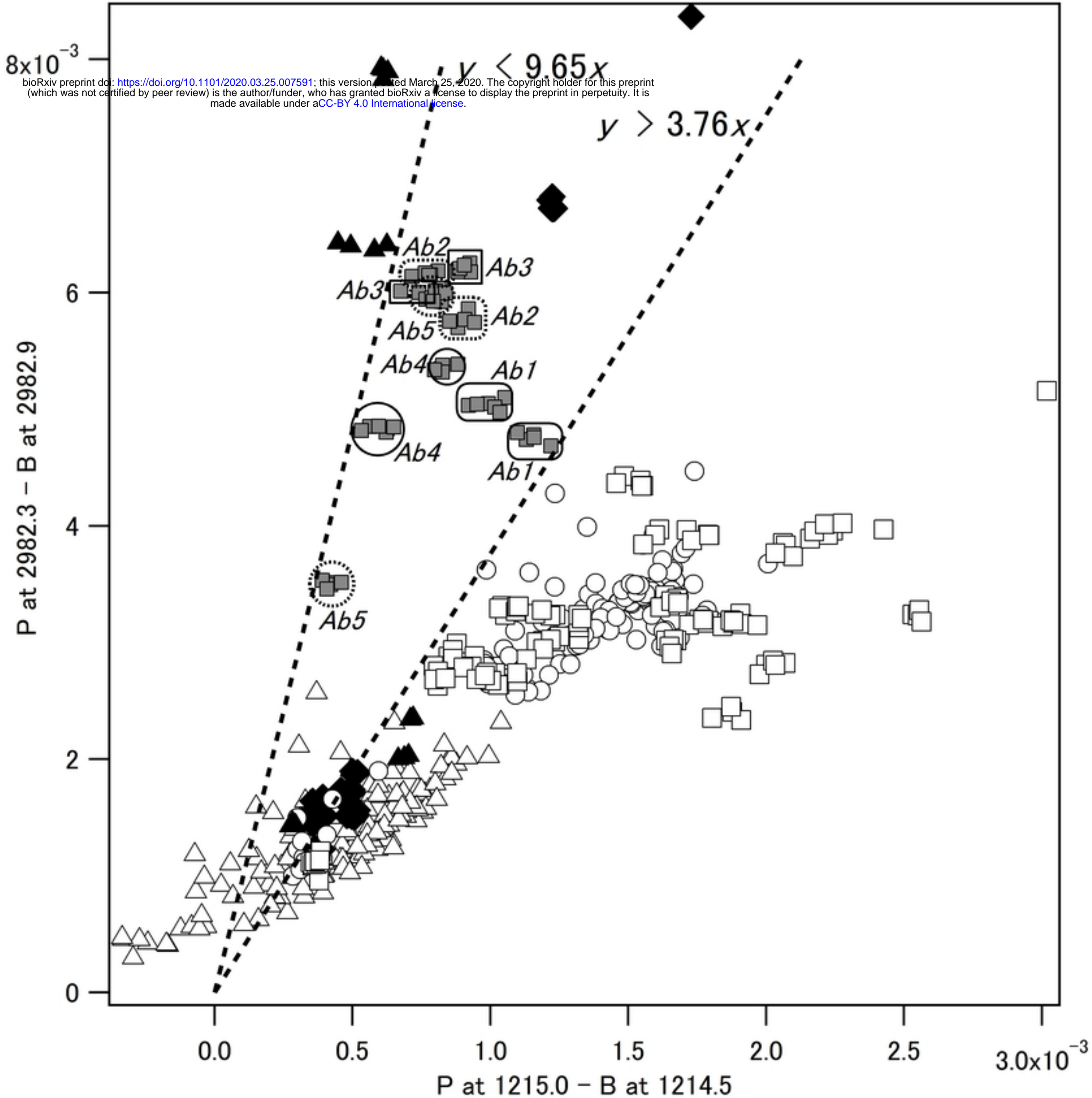


Figure 3

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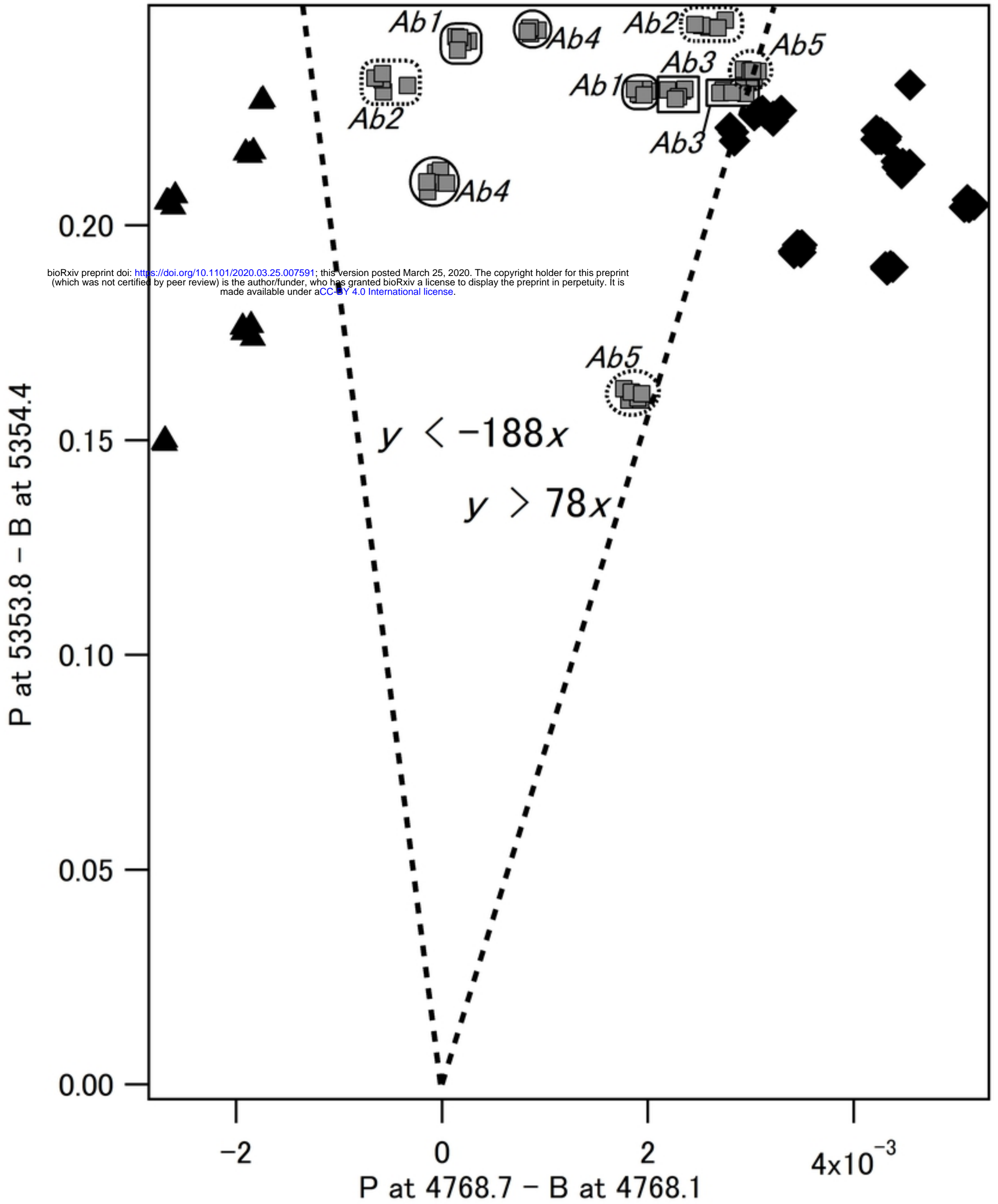


Figure 4