Brain/MINDS Beyond Human Brain MRI Study: Multi-Site Harmonization for Brain

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Abstract

Psychiatric and neurological disorders are afflictions of the brain that can affect individuals throughout their lifespan. Many brain magnetic resonance imaging (MRI) studies have been conducted; however, imaging-based diagnostic and therapeutic biomarkers are not yet well established. The Brain/MINDS Beyond human brain MRI project (FY2018 ~ FY2023) is a multi-site harmonization study aiming to establish clinically-relevant imaging biomarkers using multiple high-performance scanners, standardized multi-modal imaging, and a study design that includes traveling subjects. This project began with 13 clinical research sites that collect MRI data on psychiatric and neurological disorders across the lifespan and three research sites that design and develop measurement procedures, neuroimaging protocols, data storage and sharing, and analysis tools. Brain images obtained with the Harmonization protocol (HARP) are preprocessed and analyzed using approaches developed by the Human Connectome Project, generating preliminary cortical structure, function, and connectivity measures that are comparable across scanners. The use of 'travelling subjects', in which study participants travel to multiple sites to undergo scanning with standardized neuroimaging techniques, enable us to minimize the measurement bias between scanners and protocols and to increase the sensitivity and specificity of case-control studies. All the imaging and demographic and clinical data are shared between the participating sites and will be made publicly available in 2024. To the best of our knowledge, this is the first multi-site human brain MRI project to explore multiple psychiatric and neurological disorders across the lifespan. The Brain/MINDS Beyond human brain MRI project will help to identify the common and disease-specific pathophysiology features of brain diseases and develop imaging biomarkers for clinical practice.

<u>Keywords</u>

Multi-site Study; HCP-style Brain Imaging; Psychiatric Disorders; Neurological Disorders;

Harmonization Protocol; Traveling Subjects

Text

Abbreviations

DALYs, disability-adjusted life years

MRI, magnetic resonance imaging

HCP, Human Connectome Project

ABCD, Adolescent Brain Cognitive Development

BPD, bipolar disorder

MDD, major depressive disorder

DecNef, Decoded Neurofeedback

ASD, autism spectrum disorder

ADNI, Alzheimer's Disease Neuroimaging Initiative

AD, Alzheimer's disease

MCI, mild cognitive impairment

PPMI, Parkinson's Progression Markers Initiative

PD, Parkinson's disease

T1w, T1-weighted

T2w, T2-weighted

rsfMRI, resting state functional MRI

CRHD, Connectome Related to Human Disease

GLM, general linear model

TS, traveling subject

AMED, Japan Agency for Medical Research and Development

Brain/MINDS Beyond, Strategic International Brain Science Research Promotion Program

HARP, Harmonization protocol

DWI, diffusion-weighted imaging

QC, quality control

MNI, Montreal Neurological Institute

MSM, multi-modal surface matching

GLMM, general linear mixed model

CIFTI, Connectivity Informatics Technology Initiative

FEF, frontal eye field

PEF, premotor eye field

PSL, peri-sylvian language

STS, superior temporal sulcus

NODDI, nerite orientation and density imaging

1. Introduction

Psychiatric and neurological disorders are afflictions of the brain that can affect individuals

throughout their lifespans. Using the disability-adjusted life years (DALYs), which is a measure

of disease burden proposed by the World Health Organization Global Burden of Disease study,

in 2010 mental and behavioral disorders accounted for 7.4% of the total DALYs and

neurological disorders accounted for 3.0% (Murray et al., 2012), up from 5.4% and 1.9% in

1990, respectively. Since the 1990s, technical advances in magnetic resonance imaging (MRI)

have allowed detailed analysis of the organization of brain function and structure in humans.

Recent high-quality MRI studies with a large cohort are expected to provide neurobiological and

life-span information in healthy subjects (Glasser et al., 2016b; Harms et al., 2018; Miller et al.,

2016), which will hopefully provide diagnostic utility for patients with psychiatric and

neurological disorders (Drysdale et al., 2017; Elliott et al., 2018b; Koutsouleris et al., 2015;

Nunes et al., 2018). However, the diagnostic value of brain MRI in psychiatric disorders has not

yet been established, presumably because effect sizes tend to be small and overlap with

variability in healthy individuals (Yamashita et al., 2019). Protocols of scanning and analysis

have rarely been standardized across projects, though that has begun to change - especially for

large projects such as the Human Connectome Project (HCP; (Van Essen et al., 2012)), UK

Biobank (Miller et al., 2016), and the Adolescent Brain Cognitive Development (ABCD) project

(Casey et al., 2018).

1.1. Previous multi-site neuroimaging studies for neuropsychiatric disorders

Several brain imaging projects have attempted to identify suitable biomarkers in

neuropsychiatric diseases. Recent multi-site neuroimaging mega studies have revealed well-

replicated and clinically applicable findings from structural images; the Enhancing

NeuroImaging Genetics through Meta-Analysis Consortium in the U.S. (n = 4,568) and the

Cognitive Genetics Collaborative Research Organization in Japan (n = 2,564) replicated findings

that patients with schizophrenia have volumetric alterations of subcortical structures when

compared to healthy controls (Okada et al., 2016; van Erp et al., 2016). The findings were partly

evident in other psychiatric disorders, such as bipolar disorder (BPD) and major depressive

disorder (MDD) (Hibar et al., 2018; Schmaal et al., 2017; Schmaal et al., 2016; van Erp et al.,

2016). Using resting-state functional MRI (rsfMRI), a multi-site study successfully developed

generalized classifiers for psychiatric disorders. The Decoded Neurofeedback (DecNef) Project

(https://bicr.atr.jp/decnefpro/), a multi-site neuroimaging study in Japan (12 sites, n = 2,409),

developed a generalized classifier for autism spectrum disorder (ASD) with a high accuracy—

not only for the data in three Japanese sites (85%) but also for the Autism Brain Imaging Data

Exchange dataset (75%) (Yahata et al., 2016). The project also quantified the spectrum of

psychiatric disorders by applying the ASD classifier to other multi-disorder datasets

(schizophrenia, MDD, and attention-deficit/hyperactivity disorder). Therefore, the focus of

mega-analyses is shifting from features found in case-control studies to cross-disease

comparisons that can identify common and disease-specific features.

In the field of neurodegenerative disease, the Alzheimer's Disease Neuroimaging

Initiative (ADNI) is one of many major multi-site neuroimaging and biomarker studies of

Alzheimer's disease (AD) and mild cognitive impairment (MCI) that was started in 2005 in

North America (Mueller et al., 2005; Weiner et al., 2015). It contributed to the development of

blood and imaging biomarkers, the understanding of the biology and pathology of aging, and to

date has resulted in over 1,800 publications. ADNI also impacted worldwide ADNI-like

programs in many countries including Japan, Australia, Argentina, Taiwan, China, Korea,

Europe, and Italy. The Japanese ADNI (J-ADNI) conducted a multi-site neuroimaging study on

cognitively normal elderly patients, MCI, and mild AD (n = 537), which emphasized the

harmonization of the protocol and procedures with the ADNI (Iwatsubo et al., 2018). J-ADNI

also developed machine learning techniques using feature-ranking, a genetic algorithm, and a

structural MRI-based atrophy measure to predict the conversion from MCI to AD (Beheshti et

al., 2017). Inspired by the Parkinson's Progression Markers Initiative (PPMI; (Parkinson

Progression Marker Initiative, 2011), the Japanese (J-) PPMI team has also started a cohort in

patients with rapid eye movement sleep behavioral disorder, which is regarded to be prodromal

to Parkinson's disease (PD) (Mukai and Murata, 2017).

These previous mega-studies have contributed to the discovery of potential mechanisms

and biomarkers of multiple brain disorders. However, most of these imaging biomarkers have a

relatively small effect sizes and the study results were drawn from multi-site data which are often

heterogenous and used now outdated traditional low-resolution data acquisition protocols. In

addition, there have been no human brain MRI studies that explore multiple psychiatric and

neurological disorders that occur through the lifespan within the same cohort of subjects.

1.2. High-quality multi-modal MRI protocols and preprocessing pipelines

The HCP developed a broad approach to improving brain imaging data acquisition,

preprocessing, analysis, and sharing (Glasser et al., 2016b). It includes: 1) high-quality multi-

modal data acquisition; 2) in a large number of subjects; and 3) high-quality data preprocessing

and has proven usefulness of MRI techniques for understanding the detailed organization of a

healthy human brain (Elliott et al., 2018a; Glasser et al., 2016a; Smith et al., 2015). The HCP

aimed to delineate the brain areas and characterize neural pathways that underlie brain function

and behavior in 1,200 healthy young adults (Van Essen et al., 2012). HCP scans were performed

by a single MR scanner (a customized 3T Skyra, Siemens Healthcare GmbH, Erlangen,

Germany) in a total of 4-hour scan time for high-resolution multi-modal data, which included

T1-weighted (T1w) images, T2-weighted (T2w) images, diffusion-weighted images (DWI),

rsfMRI, and task fMRI (Glasser et al., 2016b; Glasser et al., 2013). The HCP also developed a

set of preprocessing pipelines with improved cross-subject alignment that dramatically improves

the spatial localization of brain imaging findings and also increasing statistical sensitivity

(Coalson et al., 2018; Glasser et al., 2013; Robinson et al., 2018). For the Lifespan Developing

and Aging HCP Projects (HCP-D and HCP-A) the original HCP protocol for healthy young

adults was shortened, for children and the elderly (60 to 90 min scan time; (Bookheimer et al.,

2019; Harms et al., 2018; Somerville et al., 2018), and for psychiatric and neurological disorders

(the Connectomes Related to Human Disease [CRHD];

https://www.humanconnectome.org/disease-studies), and adolescent development (the ABCD

project; (Casey et al., 2018). The UK Biobank used an even more abbreviated scanning approach

to collect a much larger number of cohort (n = 100,000) to predict health conditions (Miller et

al., 2016).

Many of these high-quality multimodal projects have been based on a single or small

number of the same model scanners at different sites and thus did not fully address

standardization of the data acquisition across different scanner models or vendors. We aim to

accelerate harmonization technologies to be used in at least five scanner platforms by combining

approaches to high-quality imaging acquisition, preprocessing, study design, and statistical bias

correction to potentially improve the sensitivity and validity of imaging biomarkers.

1.3. Traveling subjects

A harmonization approach is required for individual-based statistics using a multi-site dataset,

even when the brain images are obtained using the same machine and protocol, because the data

from each site has the bias from hardware and scanning protocol (measurement bias) and

sampling variability (i.e. age, sex, handedness, and socioeconomic status). If measurement biases

were correlated or anti-correlated with a specific disease state this would result in a positive or

negative bias in a given measure, whereas uncorrelated biases would merely reduce sensitivity

(i.e. SNR) of the measure. Sampling biases due to biological differences in the sampled

populations should also be considered for both case and control groups. Data harmonization has

been proposed to control for these biases, including a general linear model (GLM) with the site

as the covariate, a Bayesian approach (Fortin et al., 2018; Fortin et al., 2017), and a meta-

analytic approach (Okada et al., 2016; van Erp et al., 2016), but the methods used for controlling

both biases are unable to distinguish between them (Yamashita et al., 2019). Inter-site cross-

validation by machine learning and deep learning techniques is a method that aims to remove

bias without any specific preparation if large-sample datasets are available (Nunes et al., 2018).

However, this method extracts stable characteristics across the images and is limited to using

only a part of the information for further analysis. In addition, it is unclear whether the classifiers

obtained by such methods can be applied to an independent new site of the initial multi-site

project.

The traveling subject (TS) approach is a powerful research design to control for site

differences (Figure 1). This approach requires the images from the same participants at all the

participating sites, but also requires significant effort from the sites and the participants when

compared to other harmonization methods listed above, and the TS scans must be completed

before the analysis starts. However, the TS approach can differentiate most of the sample

variability from measurement bias (Yamashita et al., 2019). The DecNef Project explored

rsfMRI functional connectivity for multiple psychiatric diseases and scanned nine TS

participants who received repeated MRI measurements at all sites. Measurement and sampling

biases for each group (schizophrenia, MDD, ASD, and healthy controls) were segregated from

individual and disease-specific factors as the rest of sampling variability. The results showed that

the effects of both bias types on functional connectivity were greater than or equal to those of

disease-specific factors. With regard to measurement bias, differences in phase encoding

direction had the biggest effect size when compared to those of vendor, coil, and scanner within

the same vendor. The harmonization method was estimated to reduce measurement bias by 29%

and improve the signal-to-noise ratio by 40% (Yamashita et al., 2019). Further investigations are

needed to determine the best approach for reducing sampling bias arising from biological

differences in the sampled population.

Figure 1. Case-control studies and traveling subject approach.
(Top) When we analyze multi-site data from a set of case-control MRI studies, we must consider machine and protocol-derived bias (measurement bias) as well as sampling bias (from biological differences in the sampled populations). Even if the machine and protocol are the same between sites (e.g. Sites A and B), measurement bias may still occur because of slight differences in the magnetic or radiofrequency fields, etc. Sampling bias should be considered for patient groups as well as control groups, given that the control participants were recruited according to the demographics in the patient group. (Bottom) The traveling subject (TS) harmonization approach enables us to combine with case-control datasets by differentiating between measurement and sampling biases (Yamashita et al., 2019). Based on the general linear model (GLM), TS participants need to receive measurements from all participating sites (e.g. only TS 1 dataset). To reduce the effort of TS participants and participating sites, this project applies a general linear mixed model (GLMM) approach and hub-and-spoke model to the TS project. With this approach, all participants receive scans at one or more hub sites (site A), and measurement bias is calculated using multiple TS datasets by means of a GLMM (TS 1 and 2).

254   *1.4. Brain/MINDS Beyond project*

The Strategic International Brain Science Research Promotion Program (Brain/MINDS Beyond;

FY2018–FY2023; https://brainminds-beyond.jp/) was funded by the Japan Agency for Medical

Research and Development (AMED) to support global brain research by enhancing collaboration

with the domestic projects of other countries. Brain/MINDS Beyond consists of four research

groups: G1-1, Identification of the pathogenic mechanism of psychiatric and neurological

disorders through the acquisition and analysis of brain MRI-scan images and clinical data

(Developmental [G1-1D], adult [G1-1A], and senescent [G1-1S] stages); G1-2, Brain MRI data

acquisition, analysis, and informatics; G2, Research involving an inter-species comparison of

human and nonhuman primate brains by structural and functional parcellation and homology

analyses; and G3, Development and application of technologies, such as neuro-feedback through

collaboration with artificial intelligence research projects as well as the Innovative Research

Group. In human brain imaging, G1-1 intends to measure human participants, including patients

with neuropsychiatric disorders, across the lifespan, and G1-2 intends to coordinate and support

data acquisition, storage, preprocessing, analysis, and distribution (Figure 2 and Table 1). The

Brain/MINDS Beyond MRI working group also set up a standardized procedure for MRI data

acquisition (Harmonization protocol [HARP]) and clinical and neurocognitive data assessment

(Tables 2 and 3). Following previous multi-site studies in Japan (Iwatsubo et al., 2018; Okada et

al., 2016; Yahata et al., 2016; Yamashita et al., 2019), the overall goal is to find an altered brain

imaging characteristics in psychiatric and neurological disorders that can be applied to future

therapeutic investigations and clinical devices. To address limitations of previous findings in

multi-site studies, we are using high performance research-based MRI scanners and we modeled

our multi-modal protocol (T1w images, T2w images, diffusion-weighted imaging [DWI],

rsfMRI, task fMRI, quantitative susceptibility mapping, and arterial spin labeling) on that used

by the HCP and ABCD study projects. We are also obtaining a TS dataset for the harmonization

of the clinical MRI datasets and the development of technical tools to harmonize the multi-site

data. Once the project period ends, the data will be openly distributed to researchers via a public

database.

Here, we introduce the Brain/MINDS Beyond human brain MRI project and show

preliminary results in high-quality neuroimaging using the TS data that is amenable to

harmonization. We then discuss our plans for investigating the neural basis of psychiatric and

neurological disorders in the hope of developing therapeutic targets and devices that are

applicable to clinical settings.

Figure 2. Brain/MINDS Beyond human brain MRI project.
Institutes in the blue boxes show measurement and analysis sites for neuropsychiatric
disorders, and those in the orange boxes show analysis support sites. Institutes listed in boxes
with a colored background represent participation in the traveling subject project.

2. Brain/MINDS Beyond human brain MRI study

2.1. Participating sites and target population

As of March 2020, 13 sites have approved this study project, received approval from their

respective ethical review board(s), and obtained clinical and TS measurements using the

appropriate MRI scanners (Table 1). Of these, 5 sites mainly explore psychiatric disorders

(schizophrenia, ASD, MDD, and BPD), 4 sites neurological disorders (AD, PD, multiple system

atrophy, progressive supranuclear palsy, chronic pain disorder, and epilepsy), and 2 sites both

categories. Two sites measure the general adolescent population to investigate brain development

and recruit through advertisement and cohort studies (Ando et al., 2019; Okada et al., 2019).

Each site intends to obtain brain images and demographic (and clinical) characteristics for

clinical cases and match controls for age, sex, premorbid IQ or educational attainment, socio-

economic status, and handedness (See Cognitive and behavioral assessment section). The

exclusion criteria were set by each study purpose (i.e. low premorbid IQ, history of loss of

consciousness for more than 5 min, illegal drug use, and alcohol dependency). Illegal drug use

can be a major concern for disease onset and poor prognosis, especially for psychiatric disorders.

However, there is far less illegal drug use in Japan compared to Western European countries

(Degenhardt et al., 2008; Lee and Kwon, 2016), and most of the participating sites excluded

those with a current illegal drug use or previous history of regular use (Koike et al., 2013).

For the TS project, 75 healthy adults planned to undergo 6 to 8 scans at three or more

sites within 6 months (See Traveling Subject Project section). Five or more participants per site

were recruited. Each participant received test-retest scans at the recruitment site and underwent

scans at different sites including a hub site. We set up three hub sites, according to a hub-and-

310   spoke model, in which all participants received scans using a MAGNETOM Prisma scanner

311   (Siemens Healthcare GmbH, Erlangen, Germany) and the CRHD and HARP protocols.

312   **Table 1. Participating sites of the Brain/MINDS Beyond MRI project.**

Site	Research group	Role	MRI scanner (System version)	Protocol	Main target population
UTK	G1-1D, G1-2	Data acquisition/Analysis	Prisma (VE11C)	CRHD	Adolescent cohort, HP, ASD, Sch, MDD, Epilepsy
UTI	G1-1D, G1-2	Data acquisition/Sharing	Prisma (VE11C)	CRHD	HP, ASD, Sch, MDD, BPD
ATR	G1-2, G3	Data acquisition/Sharing/ Analysis	Prisma (VE11C)	CRHD	HP
FUM	G1-1S	Data acquisition	Skyra (VE11C)	HARP	HP, AD, PD
TMG	G1-1D	HARP setup/Data acquisition	Trio (VB19A)	HARP	Adolescent cohort
SWA	G1-1D, G3, IR	HARP setup/Data acquisition	Skyra (VE11E)	HARP	HP, ASD
NCNP	G1-1S	HARP setup/Data acquisition/Sharing/ Analysis	Verio Tim+Dot (VD13A)	HARP	HP, Sch, MDD, AD, PD
JTD	IR	Data acquisition	Prisma (VE11C)	HARP	HP, Chronic pain
UOS	G2	Data acquisition	Prisma (VE11C)	HARP	HP, PD, MSA, PSP
UHI	G1-1A, G3	HARP setup/Data acquisition	Skyra (VE11C)	HARP	HP, MDD, BPD
UNG	BM	Data acquisition	Verio (VB17A)	HARP	HP, Sch
UKY	G1-1S	HARP setup/Data acquisition	Skyra (VE11C)	HARP	HP, AD, PD
KRC	G1-1A	Data acquisition	Verio (VB17A)	HARP	HP, Sch, MDD, BPD
BDR	G1-2	HARP setup/Data Analysis	Prisma (VE11C)	HARP	NA

Abbreviations: UTK, The University of Tokyo ECS (Komaba Campus); UTI, The University of
Tokyo IRCN; FUM, Fukushima Medical University; TMG, Tamagawa Academy & University;
SWA, Showa University; NCNP, National Center of Neurology and Psychiatry; JTD, Juntendo
Hospital; ATR, Advanced Telecommunications Research Institute International; UOS, Osaka
University; UHI, Hiroshima University; UNG, Nagoya University; UKY, Kyoto University;
KRC, Kyoto University Kokoro Research Center; BDR, RIKEN Center for Biosystems
Dynamics Research; IR, Innovative Research Group in Brain/MINDS Beyond; BM,
Brain/MINDS project; CRHD, Human Connectome Studies Related To Human Disease protocol;
HARP, harmonization protocol; HP, healthy participants; ASD, autism spectrum disorders; Sch,
schizophrenia; MDD, major depressive disorder; BPD, bipolar disorder; AD, Alzheimer's
disease; PD, Parkinson disease; MSA, multiple system atrophy; PSP, progressive supranuclear
palsy.
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2.2. Harmonized brain MRI protocols

We developed protocols that minimize potential differences related to measurement and increase

the MR image sensitivity to brain organization in psychiatric and neurological disorders. From a

neurobiological perspective, the cerebral cortex is organized by a 2D sheet-like structure with an

average thickness of 2.6 mm embedded and folded in the ~1300 mL of brain volume (Glasser et

al., 2016b). From a neuroimaging perspective, the spatial resolution and homogeneity of the

images are important factors that may induce bias and error during the image analysis; these

include partial voluming, image distortion, errors in brain segmentation, and registration. Of

these, respecting spatial fidelity of neuroanatomical structures is the most important approach for

achieving unbiased imaging (Glasser et al., 2016b). Therefore, the spatial resolution of the

imaging was determined based on cortical thickness and was matched across all scanners. The

phase encoding direction of EPI-based functional and diffusion MRI is an important factor that

relates to spatial distortion (and signal loss in fMRI) in association with the polarity of the

direction, echo spacing, and B0 magnetic field homogeneity; therefore, we acquire a spin-echo

filed map with opposing phase encoding directions to enable distortion correction (Andersson et

al., 2003). Based on these strategies, two MRI protocols were planned for use in the project: 1) a

harmonized MRI protocol (HARP), which can be run on the multiple MRI scanners/sites within

a period of 22 to 65 min; and 2) an 'HCP style' MRI protocol used by HCP CRHD for the high-

performance 3T MRI scanner (e.g. MAGNETOM Prisma).

The HARP was created to be used at multiple MRI scanners/sites, and it was designed to

obtain high-quality and standardized brain MRI data in a 'clinically' practical window of time

(Table 2 and Supplementary Table S1). The parameters of the MRI scanners were as follows: 1)

static magnetic field strength of 3T; 2) multi-array head coil with 32 or more channels; and 3)

ability to perform a multi-band EPI sequence provided from Center for Magnetic Resonance

Research, University of Minnesota with an acceleration factor of 6 (Moeller et al., 2010;

Setsompop et al., 2012; Xu et al., 2013). In 2019, the protocol was adapted for use with five MRI

scanners/systems (MAGNETOM Prisma, Skyra, Trio A Tim, Verio, and Verio Dot; Siemens

Healthcare GmbH, Erlangen, Germany), and we plan to expand it to different MRI

scanners/vendors during the project period. The HARP was intended to perform the brain scan

within a period of ~ 30 min using a high-resolution structural MRI scan (T1w and T2w, spatial

resolution of 0.8 mm) and two high-sensitive rsfMRI scans with opposing phase directions, a

spatial resolution of 2.4 mm, and a temporal resolution of 0.8 s for a total of 10 minutes. The

protocols also include optional sequences for four additional rsfMRI scans, task fMRI (Emotion

and CARIT) (Winter and Sheridan, 2014), two DWI scans with opposing phase encoding

directions, quantitative susceptibility mapping, and arterial spin labeling. The minimum and

maximum scanning time of the HARP is 22 and 65 min, respectively (Table 2). The preliminary

results across scanners and multi-array coils in the same subject (ID = 9503) revealed that the

temporal signal-to-noise ratio (tSNR) was very high in all the scanners. The mean ± standard

deviation across 32k greyordinates was 161 ± 80 in the Prisma at UTK, 155 ± 81 in the Verio

Dot at SWA, 151 ± 72 in the Skyra fit at SWA, 151 ± 80 in the Verio at ATR, and 150 ± 74 in

the Prisma fit at ATR; the values and their distributions were similar across scanners/sites

(Figure 3A).

The CRHD protocol was planned for collaboration with the HCP CRHD for the Early

Psychosis Project. The HCP CRHD protocol also included high-resolution structural MRI

(spatial resolution of 0.8 mm), high-resolution resting-state fMRI (spatial resolution of 2 mm)

with an opposing phase encoding direction and longer scan time, and high-resolution and high

angular diffusion MRI.

The installation of the protocols in the MRI scanners was ensured by conducting

hierarchical parameter checks and site visits at the beginning of the measurement period. After

the protocol installation, each site sent XML files of the installed protocol from the MRI scanner

to the protocol management site (UTK), and all the parameters were confirmed with a checksum

algorithm using R (R Core Team, 2018). This process was useful for validating the protocols

across sites/scanners because some of the MRI scanners actually underwent inappropriate

installation and were set with different parameters. The results were then sent back to the

collaborators, who edited the parameters. We also checkrf the DICOM files that are deposited in

the ATR XNAT server. In this phase, we checked the parameters, slice numbers, and diffusion

gradient information (bvec and bval).

The manuals were shared and used at the sites for protocol installation, demographic and

clinical assessment before the scan (e.g. handedness), and the assessment of and instruction to

participants during the scan (e.g. general instruction during the scan, fixation to the cross during

rsfMRI scans, and the assessment of sleepiness during the rsfMRI).

Table 2. CRHD and HARP protocols.

Subset	Sequence	Duration			Participant instruction
		Prisma		Skyra, Trio, Verio Dot, Verio	
		CRHD	HARP	HARP	
rsfMRI 1	SEF AP	0:32	0:06		Fixation
	BOLD AP	5:46	5:08		Fixation
	SEF PA	0:32	0:06		Fixation
	BOLD PA	5:46	5:08		Fixation
Structure	T1 MPR	6:38	5:22		Rest
	T2 SPC	5:57	5:31	5:22-6:26	Rest
Subtotal		**25 min**	**22 min**	**22-23 min**	
ASL		NA	2:45[b]		Rest
QSM		NA	5:03[c]		Rest
DWI	AP	6:07	3:29	4:50	Rest
	PA	6:05	3:32	4:54	Rest
	AP	5:39	NA	NA	Rest
	PA	5:39	NA	NA	Rest
rsfMRI 2	See rsfMRI 1[a]	13 min	11 min		Fixation
rsfMRI 3	See rsfMRI 1[a]	NA	11 min		Fixation
Task fMRI EMOTION	SEF AP	NA	0.06		Task
	SEF PA	NA	0.06		Task
	BOLD PA	NA	4.08		Task
Task fMRI CARIT	SEF AP	NA	0.06		Task
	SEF PA	NA	0.06		Task
	BOLD PA	NA	4.08		Task
Total		**61 min**	**68 min**	**59-68 min**	

Abbreviations: rsfMRI, resting-state functional MRI; ASL, arterial spin labeling; QSM,

quantitative susceptibility mapping; DWI, diffusion weighted imaging; SEF, spin echo field

mapping; BOLD, blood oxygenation level dependent; T1 MPR, T1-weighted magnetization

prepared rapid acquisition with gradient echo; T2 SPC, T2-weighted sampling perfection with

application optimized contrasts using different flip angle evolutions.

a A set of SEF AP, BOLD AP, SEF PA, and BOLD PA.

b Only for Prisma and Skyra.

c Only for Prisma, Skyra, and Verio Dot.

Figure 3. Quality of MRI and preliminary cortical structures obtained by HARP in a single traveling subject across scanners/sites.

A) Temporal signal-to-noise ratio (tSNR) obtained in a single subject (ID = 9503) across different scanners/sites by a harmonized MRI protocol (a sequence of functional MRI in HARP using a multi-band echo planar imaging with TR/TE = 800/34.4 ms; see Supplementary Table S1 for other details). The images from top to bottom show color-coded tSNR maps in 32k greyordinates (see main text) overlaid on the lateral and medial surface of the mid-thickness surface of the left hemisphere, the subcortical sections of the T1w image, and the histogram of the tSNR values. B) Cortical myelin contrast (T1w/T2w ratio) across different scanners. The myelin contrast is corrected for the biasfield and parcellated by the HCP MMP v1.0 (Glasser et al., 2016a). C) The map shows cortical thickness across different scanners. Cortical thickness is corrected by curvature and parcellated by the HCP MMP v1.0. The tSNR, myelin map and cortical thickness are comparable across scanners. Data at https://balsa.wustl.edu/7q4P9 and https://balsa.wustl.edu/6Vvqv

2.3. Cognitive and behavioral assessment

Each participating site assesses demographic characteristics (i.e. age, sex, and socioeconomic

status), clinical characteristics (i.e. diagnosis, symptom severity, cognitive function, and general

functioning), and subjective social evaluations (i.e. quality of life and well-being) (Table 3).

Each subgroup (G1-1D, G1-1A, G1-1S, and G1-2 TS) indicates standard scales, some of which

are uniform across subgroups and easier to share and use when analyzing brain images.

Table 3. Clinical and neuropsychological assessment.

	G1-1D	G1-1A	G1-1S
Depression	K6 or BDI-II	BDI-II and PHQ-9	PHQ-9 and BDI-II/GDS-15
Anxiety	—	GAD-7	STAI
Autism	AQ-10, AQ-50 or SRS-2 (for developmental disorders)	AQ-10 or AQ-50	—
Psychosis	APSS	—	NPI-Q
Intellectual ability	JART-25 or WAIS-III (WISC at the age of 15 years or less) Information and Picture completion subtests	JART-25	JART-25
Cognitive function	CANTAB or BACS-J	CANTAB or BACS-J	ADAS-Cog11, CDT, CDR, FAB, HVLT-R, JLO, MMSE, MoCA-J, SDMT, TMT-A/B, WMS-R
General function and disability	GAF, mGAF or WHO-DAS 2.0	GAF, mGAF or WHO-DAS 2.0	Schwab & England ADL
Quality of life	EQ-5D	EQ-5D	PASE
Well-being	WHO-5	WHO-5	SHAPS
Handedness	EHRS or UTokyo	EHRS or UTokyo	UTokyo

Abbreviations: K6, 6-item Kessler Screening Scale for Psychological Distress; BDI-II, Beck Depression Inventory－Second Edition; PHQ-9, Patient Health Questionnaire-9; GDS-15, Geriatric Depression Scale 15; GAD-7, General Anxiety Disorder-7; STAI, State-Trait Anxiety Inventory; AQ-10, 10-item short version of the Autism Spectrum Quotient; AQ-50, Autism Spectrum Quotient (original version); APSS, Adolescent Psychotic-like Symptom Screener; NPI-Q, Neuro Psychiatric Inventory-Brief Questionnaire Form; JART-25, 25-item short version of the Japanese Adult Reading Test; WAIS-III, Wechsler Adult Intelligence Scale－Third Edition; GAF, Global Assessment of Functioning; mGAF, modified GAF; WHO-DAS 2.0, the World Health Organization Disability Assessment Schedule II; Schwab & England ADL, Modified Schwab and England ADL (Activities of Daily Living) scale; CANTAB, Cambridge Neuropsychological Test Automated Battery; BACS-J, the Brief Assessment of Cognition in Schizophrenia Japanese version; ADAS-Cog, Alzheimer's Disease Assessment Scale-cognitive component; CDT, Clock Drawing Test; CDR, Clinical Dementia Rating; FAB, Frontal Assessment Battery; HVLT-R, Hopkins Verbal Learning Test-Revised; JLO, Judgment of Line Orientation; MMSE, Mini-Mental State Examination; MoCA-J, Japanese version of Montreal Cognitive Assessment; SDMT, Symbol Digit Modality Test; TMT-A/B, Trail Making Test Parts A and B; WMS-R, Wechsler Memory Scale-Revised; EQ-5D, EuroQol 5 Dimension questionnaire; WHO-5, World Health Organization-Five Well-Being Index; PACE, Physical Activity Scale for Elderly; SHAPS, Snaith-Hamilton Pleasure Scale; EHI, Edinburgh Handedness Inventory; UTokyo, 14-item Rating Scale of Handedness for Biological Psychiatry Research among Japanese People.

2.4. Travelling subject project

Based on the previous study (Yamashita et al., 2019), we also conducted a TS project for the

CRHD and HARP protocols. In some sites, we also use the former protocols to combine with

existing large-scale datasets (Iwatsubo et al., 2018; Okada et al., 2016; Yahata et al., 2016;

Yamashita et al., 2019). Because we limit the scanners, head coils, and protocols in this project,

we expect to see reduced measurement biases, which may enhance the disease-related effect size

in clinical studies and provide better ways to diminish bias in future studies.

The previous data harmonization using the TS dataset was based on a GLM (Yamashita

et al., 2019); however, the present TS project may provide a harmonization method using a

general linear mixed model (GLMM; Figure 1), given that the new protocols require a longer

scan time compared to previous protocols (~20 min for T1w imaging and rsfMRI). To ensure the

images from all sites are well harmonized, we applied a hub-and-spoke model to arrange

traveling scans at each recruitment site (Supplementary Table S2). Each participant undergoes

CRHD and HARP scans using the Prisma (~2 hours) at one or more hub sites (UTK, UTI, and

ATR) to harmonize the data within the Brain/MINDS Beyond project and other projects (e.g.

Brain/MINDS, HCP, and ABCD) and test the difference in quality between the protocols. The

other visiting sites were determined in consideration of the site locations, machine differences,

and project similarities between the sites. Each participant receives multiple scans at the

recruitment site to assess the test-retest reliability (1 hour x 2 sessions). The interval between

scans may vary by site due to scanner time restrictions but we aim to determine whether the gap

between test-retest scans would be associated with reliability.

For the TS project, 75 healthy adults—five or more participants per site—are scheduled

to undergo 6 to 8 scans at three or more sites within 6 months (Supplementary Table S2). The

total number of scans and spokes between the sites are expected to be 455 and 465, respectively

(Figure 4A). As of March 2020, 74 participants were registered and 405 scans (89.0 %) were

completed and uploaded to the ATR XNAT server. The data provided 368 spokes (76.1 %,

Figure 4B). The TS project will end in August 2020.

We also plan another TS project including task fMRI sequences in HARP to see the

validity and reliability of the task fMRI paradigms and the applicability of harmonizing higher

quality registration using the task fMRI data. The task fMRI TS study is set to begin September

2020 and will include 10 participants, 4 sites (UTK [including test-retest], UTI, TMG and SWA),

and a total of 50 scans.

Figure 4. Expected and current data connection of the traveling subjects.
Data connections in the traveling subject project that were (A) initially planned and (B) the
actual connections as of March 2020. Hub sites using Prisma and other sites using Prisma, Skyra,
Trio A Tim, Verio Dot, and Verio are illustrated in red, orange, blue, green, purple, and pink,
respectively.

458 *2.5. Data storage, preprocessing, and quality control*

2.5.1. Data logistics

Brain MR images obtained using the CRHD and HARP protocols in this study project and related studies are stored, preprocessed, and distributed using the XNAT server system (https://www.xnat.org/) (Figure 5). Due to the legacy of previous multi-site studies (Iwatsubo et al., 2018; Yahata et al., 2016; Yamashita et al., 2019), several data centers were already available for this project. The images obtained from the development and adult projects (G1-1D and G1-1A) will be sent to an XNAT server at ATR and the clinical data will be sent to UTI. For the senescent project (G1-1S), all the data will be sent to the NCNP (Iwatsubo et al., 2018). The TS data will also be sent to the ATR server shown in dashed lines. When uploading to the XNAT server, personal information (i.e. name and date of birth) contained in DICOM is automatically removed using an anonymization script of XNAT. A defacing procedure is performed for T1w and T2w images. These processes de-identify the MRI data. After manually checking whether the face images are completely obscured, all the anonymized MRI data are shared using Amazon AWS with RIKEN BDR, in which all image preprocessing is performed (See Preprocessing pipelines section). Preprocessed data are sent back to the servers and can be seen with limited access (i.e. participating sites). After a quality control (QC), cleaned imaging data with a demographic and clinical datasheet will be stored in the distribution server(s). All data will be also sent to backup server(s).

Figure 5. Data storage, preprocessing, quality check, and data sharing.
MRI (black line) and clinical (blue line) data from G1-1D and G1-1A sites are sent to the XNAT server and a data server at ATR and UTI, respectively. All data from G1-1S sites are sent to an XNAT server and a data server managed by NCNP, as this group applied a standard clinical assessment protocol to the project following a previous multi-site study. Traveling subject data from G1-1S sites are also sent to the XNAT server in ATR (dot line). XNAT servers at NCNP, ATR, and RIKEN BDR are linked by Amazon AWS to share the imaging data. NCNP manages a separate server for storing clinical data (Clin DB) being collected from the participants in this project. All MR images are preprocessed at RIKEN BDR. All MR images are preprocessed at RIKEN BDR. All of the raw and preprocessed data will be stored and provided to the users in a distribution server. A backup server will be placed at a different site.

2.5.2. Preprocessing pipelines

All neuroimaging data are preprocessed at RIKEN BDR for this project. The MR images are sent

via Amazon S3 to a high-throughput parallel computing system at RIKEN BDR for

preprocessing. The preprocessing is performed using the HCP pipeline 4.2.0 (Glasser et al.,

2013) with modifications for adapting and harmonizing multiple scanners. In brief, the structural

MRI (T1w and T2w) is first corrected for image distortions related to the gradient nonlinearity in

each scanner type and the inhomogeneity of the B0 static magnetic field in each scan. The signal

homogeneity is dealt with by prescan normalization and is also improved by a biasfield

correction using T1w and T2w images (Glasser and Van Essen, 2011). The T1w and T2w

images are fed into non-linear registration to the Montreal Neurological Institute (MNI) space

and used for cortical surface reconstruction using FreeSurfer (Fischl, 2012), surface registration

using multi-modal surface matching (MSM) (Robinson et al., 2018) and folding pattern

(MSMsulc); this is followed by the creation of a myelin map using T1w divided by T2w and

surface mapping (Glasser and Van Essen, 2011). An example of a cortical myelin map in a single

subject (ID = 9503) across scanners/sites is parcellated by HCP MMP v1.0 (Glasser et al., 2016a)

and presented in Figure 3B, revealing the typical cortical distribution of the high myelin contrast

in the primary sensorimotor (aeras 1, 3a, 3b, 4), auditory (A1), visual (V1), middle temporal, and

ventral prefrontal (47m) areas—as demonstrated previously (Glasser and Van Essen, 2011), and

is quite comparable between scanners.

The functional MRI data is corrected for distortion (gradient nonlinearity and B0-

inhomogeneity) and motion. The distortion from B0 static field inhomogeneity is corrected by

means of opposite phase encoding spin echo fieldmap data using TOPUP (Andersson et al.,

2003); it is then warped and resampled to MNI space at a 2 mm resolution and saved as a volume

in the Neuroimaging Informatics Technology Initiative (NIFTI) format. The region of the

cortical ribbon in the fMRI volume is further mapped onto the cortical surface and combined

with voxels in the subcortical gray region to create 32k greyordinates in the Connectivity

Informatics Technology Initiative (CIFTI) format. Multiple runs of the fMRI data are merged

and fed into independent component analyses (ICA) followed by an automated classification of

noise components and the removal of noise components using FIX (Salimi-Khorshidi et al.,

2014) (Glasser et al., 2018). The automated classifier is trained using the data in this project and

its accuracy is maximized. The denoised fMRI data, in combination with other cortical metrics

(myelin, thickness; Figure 3B and 3C, respectively), is further used for multi-modal registrations

(MSMAll) over the cortical surface, followed by 'de-drifting' (removing registration bias after

multimodal registration) based on the group sampled in this study (Glasser et al., 2016a). The

resting-state seed-based functional connectivity in an example of a single subject (ID = 9503)

revealed a typical pattern over the cerebral cortex across scanners/sites; the left frontal eye field

(FEF)-seed functional connectivity showed symmetric coactivation in the bilateral premotor eye

field (PEF) (Figure 6A), whereas the left area 55b-seed FC showed an asymmetric language

network distributed in the peri-sylvian language (PSL) area, superior temporal sulcus (STS), and

areas 44/45 predominantly in the left hemisphere (Figure 6B).

518   The diffusion MRI is corrected for distortion and motion due to gradient nonlinearity,

eddy current, motion, and B0 static field inhomogeneity using EDDY (Andersson and

Sotiropoulos, 2016). The signal dropouts, susceptibility artefact, and their interaction with

motion were also corrected (Andersson et al., 2018; Andersson et al., 2017). The resulting

diffusion volumes are merged into a single volume and resampled in the subject's real physical

space aligned according to the ACPC convention. Diffusion modeling is performed using nerite

orientation density imaging (NODDI) (Fukutomi et al., 2018; Zhang et al., 2012), and a Bayesian

estimation of crossing fibers (Behrens et al., 2003; Sotiropoulos et al., 2016). Diffusion

probabilistic tractography (Behrens et al., 2003) is also performed in a surface-based analysis

(Donahue et al., 2016).

Figure 6. Seed-based resting-state functional connectivity in a single traveling subject across scanners/sites

In a single subject (ID = 9503), the resting-state fMRI scans (5 min x 4) were collected using a scanning protocol of HARP across different scanners/sites (see Supplementary Table S1), preprocessed, and denoised by a surface-based analysis to generate parcellated functional connectivity (FC) using the HCP MMP v1.0 (Glasser et al., 2016a). A) FC seeded from the left frontal eye field (FEF), which was distributed symmetrically in the bilateral premotor eye field (PEF) and comparable across scanners/sites. B) FC seeded from the left area 55b, which showed an asymmetric language network predominant in the left hemisphere that was comparable across scanners/sites. The language network is distributed in the areas of 44/45, superior temporal sulcus, dorsal posterior part (STSdp), and peri-sylvian language (PSL). Data at https://balsa.wustl.edu/1B9VG and https://balsa.wustl.edu/5Xr71

2.5.3 Preliminary travelling subject data

Here, we show the preliminary results obtained from the initial TS data (as detailed in section

2.4). In the initial TS study, five healthy subjects participated and travelled across five sites and

received MRI scanning with HARP in different scanners, and four of them completed all the

travelling scans as planned. Datasets were analyzed with the current version of preprocessing

(see section 2.5.2) and each of the cortical thickness, myelin, and resting-state functional

connectivity was parcellated using HCP MMP v1.0 (Glasser et al., 2016a) as described above (a

part of the parcellated data in an exemplar subject [ID = 9503] was already shown in Figure 3

and 6). To investigate similarity of the data, each of the parcellated metrics was fed into an

analysis of Spearman's rank correlation across subjects and sites/scanners. Figure 7 shows the

resultant similarity matrices which demonstrate higher correlation coefficients of within-subjects

than those of cross-subjects in all the metrics of cortical thickness, myelin, and functional

connectivity. These findings suggest that our approach with harmonized protocols and

preprocessing is promising for capturing a subject-specific imaging biomarker.

Figure 7. Similarity of the cortical metrics across subjects and sites/scanners in preliminary travelling subject study
From left to right show the correlation matrices of the parcellated cortical thickness, myelin and functional connectivity in four travelling subjects (TS). Number of parcellated metrics

used for analysis were 360 for thickness and myelin and 129,240 for functional connectivity, which cover all the cerebral cortex in both hemispheres. The correlation coefficient of Spearman's rho is presented by a color bar placed at the bottom.

2.5.4. Quality control

QC is implemented in several stages: 1) a brief image check during each scan; 2) an anomaly and

abnormality inspection by the radiologists; 3) an assessment of raw data image quality when

uploading data to the XNAT server; and 4) preprocessed image quality checks. QC 1 is

conducted by site personnel and the participants are rescanned within the same session if scan

time remains, if the images have major artifacts, such as those due to head movement. QC 2 is

conducted by radiologists at the measurement site or other sites if any radiologist at the site is

unable to check the images. QC 3 is manually conducted by researchers at the measurement sites

before uploading the data to a server for all images in reference to the HCP QC manual (Marcus

et al., 2013). After uploading the images to the XNAT servers, all images are first checked

according to the DICOM file information as to whether the images are correctly updated. The

researchers at each site are informed of missing DICOM files and any irregular parameters

detected in the DICOM files. In QC 3, the T1w and T2w images are manually checked as to

whether the face images are completely removed. Then, signal distributions of the myelin map

are checked for outliers because of its sensitivity to several artifacts and errors such as motion,

reconstruction of the images, and cortical surface reconstruction. Functional and diffusion

images are automatically checked for outliers, and the images and data will be checked by visual

inspection. In the QC 3 process, a QC pipeline will be implemented for checking the images

(Marcus et al., 2013). QC 4 uses preprocessed CIFTI images that will be checked in several

preprocessing steps. Any irregular scans and remarks are recorded in the clinical data servers and

the information will be used when determining the eligibility criteria for each study.

2.6. Ethical regulation

Sharing neuropsychiatric patient data, which may contain information linked to subjects'

privacy, requires special attention (Sadato et al., 2019). Therefore, the Brain/MINDS Beyond

project put NCNP as the core site for supporting ethical considerations. Before participating in

the project, all institutions are required to receive approval from their ethical review board

regarding their research plans. This includes the following points and ethical documentation: 1)

MR images and clinical data of the participants may be shared within the Brain/MINDS Beyond

project or Japanese/International scientific institutions for collaboration. De-identified MR

images with limited clinical data (see below) may become publicly accessible on an open

database for research purposes. 2) MR images of the participants may be compared with non-

human primate MRI data. 3) Intellectual property rights originating from the research of the

Brain/MINDS Beyond project shall be attributed to the institutes of the researchers and not the

participants. All participants must provide written informed consent to participate in this project

after receiving a complete explanation of the experiment.

The Japanese regulations for the sharing of personal information used for research

purposes requires attention in dealing with two types of data: "individual identification codes"

and "special care-required personal information"

(http://www.japaneselawtranslation.go.jp/law/detail/?id=2781&vm=04&re=01). Individual

identification codes are direct identifiers—information sufficient to identify a specific individual.

Special care-required personal information represents indirect identifiers needing special care in

handling so as not to cause potential disadvantages to participants. In consideration of these

regulations, data accompanied with the MR images are limited in the publicly accessible open

database, and only include 5-year age bins, sex, diagnostic information, handedness, simple

socioeconomic status, clinical scale scores, and sleepiness scale scores. In the Brain/MINDS

Beyond project, we exclude the datasets of MR images containing facial information from the

data in the publicly accessible open database.

2.7. Data sharing

In the current provisional plan of sharing the collected data, we have designated three types of

data sharing:

1) Access via an open database: de-identified MR images and limited clinical data are to become

publicly accessible for research purposes after the research period ends. The initial release will

be scheduled in 2024. Basic demographic and clinical characteristics such as 5-year age bin, sex,

socioeconomic status, (premorbid) estimated intellectual quotient, main diagnosis, representative

scale scores for each disease and sleepiness during rsfMRI scan will be shared.

2) Application-based sharing: MR images and the clinical datasets are shared after receiving

application approval for data usage by the Brain/MINDS Beyond human brain MRI study

working group. Applicants are required to obtain approval of their research plan from the ethical

review board of their institution and request the dataset type in the application form. The

working group discusses the eligibility of the applicants, as well as the availability of the

requested dataset, the ethical consideration in the Brain/MINDS Beyond site(s), and any conflict

from other applications. Data is released from the distribution server of the Brain/MINDS

Beyond project with limited access.

3) Collaboration-based sharing: This form of sharing is used for individual collaborative studies.

A research proposal collaborating with the institute(s) in the Brain/MINDS Beyond project is

approved by the ethical review board of the institute(s). Data is shared from the relevant

institute(s).

3. Discussion

The Brain/MINDS Beyond human brain MRI study expands upon research from previous multi-site neuroimaging studies in Japan and provides high quality brain images by standardizing multiple MRI scanners and protocols. An unbiased and quantitative assessment of cortical structure and function may be needed for sensitive and specific predictions of any dynamics, perturbations, or disorders of the brain system. Multi-modal cross-disease image datasets are systematically and properly acquired, analyzed, and shared to enable investigation of common and disease-specific features for psychiatric and neurological disorders with a high sensitivity and specificity. A distinct feature of this project is to include a study design with the TS project, which enables harmonizing the multi-site data from lower (i.e. preprocessing) to higher levels (i.e. statistics). The harmonization protocols are available at http://mriportal.umin.jp. The Brain/MINDS Beyond human brain MRI project can provide brain imaging biomarkers that are applicable to therapeutic targets and diagnostic supports.

To date, several national projects have applied high-quality multimodal MRI protocols, in addition to a preprocessing pipeline, to a large cohort (e.g., HCP, UK biobank, and ABCD). Unlike these multi-site projects, we plan to investigate brain organization associated with brain disorders that occur throughout the lifespan and to develop imaging biomarkers that can be implemented in clinical trials. To facilitate the collection of a larger number of patients with different brain disorders, multiple clinical research sites are participating in this project and cooperating for standardized data acquisitions. The core of the project began from establishing a standardized protocol (i.e. HARP) based on five 3T MRI scanners, but it will continue to develop a comparable protocol for other types of scanners/vendors. The protocol is designed not only for high-resolution structural MRI and high-quality resting-state fMRI, but also for diffusion MRI

and other imaging—including scans for correcting distortions. The preprocessing is performed

with a surface-based multi-modal analysis to minimize bias largely generated from the variability

in cortical folding across subjects (Coalson et al., 2018; Glasser et al., 2016b). The preliminary

data demonstrated high quality MRI images and the fidelity of structural and functional brain

organizations across scanners/sites. The signal-to-noise ratio of MRI images was very high

across scanners/sites (Figure 3A). The cortical metrics of structure (myelin map, thickness)

(Figure 3B-C) were comparable to those previously reported in the literature (Fischl and Dale,

2000; Glasser and Van Essen, 2011), as well as the functional connectivity related to eye

movements involving FEF and PEF (Figure 6A) (Amiez and Petrides, 2009) and a language

network involving left 55b, 44/45, STS, and PSL (Figure 6B) (Glasser et al., 2016a). These

findings suggest that a surface-based parcellated analysis may provide useful and reliable metrics

concerning cortical structure, function, and connectivity, and may potentially contribute to the

establishment of multi-modal imaging biomarkers of brain disorders. The initial trial with four

TS also demonstrated sensitivity to the subject-specific features across scanners/sites (Figure 7),

suggesting the reliability of our harmonizing protocols and preprocessing.

The TS approach is a novel harmonization method for multi-site brain image data

(Yamashita et al., 2019), which has proven that measurement bias from MRI equipment and

protocols can be differentiated from sampling bias between sites. Instead of using a previously

applied GLM, we plan to expand the statistical approach to a GLMM in this project. One of the

obstacles of the GLMM approach is that it requires a larger number of total scans compared to

those in a GLM approach; overlapping scans at hub sites are required for all TS participants to

ensure the data connectivity; additionally, a larger number of TS participants is required in the

TS project because the degree of freedom can be reduced in the GLMM. However, one of the

benefits of the GLMM approach includes that it is flexible with the variability in data

acquisition—such as the number of scans per participant and length of scan time per protocol;

thus, is suitable for a big project. Furthermore, this approach allows the addition of another site,

scanner, and protocol to an existing TS network, which can deal with the future upgrades of

scanners and protocols. In fact, the scanners at two sites (UHI and SWA) were upgraded to a

MAGNETOM Skyra fit (Siemens Healthcare GmbH, Erlangen, Germany) for institutional

reasons after the Brain/MINDS Beyond project had started. Therefore, we customized the TS for

two sites to ensure that the data are properly connected before and after the upgrades. Also, the

project welcomes other sites to participate in the TS network.

Because this project focuses on various brain disorders across the lifespan, we aim to

identify common and disease-specific features of psychiatric and neurological disorders. While

some case-control studies suggest possible neural mechanisms in a psychiatric disease, other

studies suggest that the effects may not be specific to a single entity but instead may be shared

across multiple neuropsychiatric disorders (Hibar et al., 2018; Schmaal et al., 2017; Schmaal et

al., 2016; van Erp et al., 2016). Such non-specificity may be at least partly addressed by

investigating diseases across the lifespan, since some of brain changes reported in psychiatric

disorders also occur in aging or development in healthy subjects, e.g. volumetric changes in

subcortical structures in schizophrenia (Okada et al., 2016; van Erp et al., 2016) and in healthy

aging (O'Shea et al., 2016; Wang et al., 2019). We initially coordinated with 13 sites to explore

various psychiatric and neurological disorders throughout the lifespan and to make use of a

powerful harmonization method. Therefore, this project aims to identify both the common and

disease-specific pathophysiology features of psychiatric and neurological disorders, which will

hopefully lead to imaging biomarkers for general clinical practice and the development of

candidate therapeutic targets for future clinical trials.

In conclusion, the Brain/MINDS Beyond human brain MRI project began with the

participation of 13 clinical research sites—all of which have setup brain image scans using the

standard MRI scanners and protocols, conducted TS scans, and will share acquired data with the

project and the public in the future, and commit to the analysis and publication of the data. To

the best of our knowledge, this is the first human brain MRI project to explore psychiatric and

neurological disorders across the lifespan. The project aims to discover robust findings which

may be directly related to the common or disease-specific pathophysiology features of such

diseases and facilitate the development of candidate biomarkers for clinical application and drug

discovery.

Acknowledgment

This research was supported by the Agency for Medical Research and Development (AMED)

under Grant Numbers JP20dm0307001 (K.K.), JP20dm0307002 (Y.O.), JP20dm0307003

(T.Han.), JP20dm0307004 (K.K.), JP20dm0307008 (M.K.), JP20dm`0307020 (N.S.),

JP20dm0207069 (S.K.) and JP20dm0307006 (T.Hay.). This study was also supported by the

University of Tokyo Center for Integrative Science of Human Behaviour (CiSHuB) and the

International Research Center for Neurointelligence (WPI-IRCN) at the University of Tokyo

Institutes for Advanced Study (UTIAS).

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Conflict of interest

Katsutoshi Murata and Yuta Urushibara are employed by Siemens Healthcare K.K., Tokyo,

Japan. The other authors report no financial relationships with commercial interests.

<u>Data availability</u>

The data presented in Figure 3 and 6 are available at BALSA

(https://balsa.wustl.edu/study/show/npD26). Harmonization protocols and other information of the

project are available at the BrainMINDS beyond MRI portal site

(http://mriportal.umin.jp/?lang=en). See also Data sharing section in details of data obtained in

future in this project. For proposal and requests for the data usage, please contact to Saori Tanaka

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