Impact of Concatenating fMRI Data on Reliability for Functional Connectomics

Jae Wook Cho[1], Annachiara Korchmaros[1], Joshua T Vogelstein[2], Michael Milham[1], Ting Xu[1]*

1. The Child Mind Institute, 101 East 56th Street, New York, NY, 10022, USA.
2. Department of Biomedical Engineering, Institute for Computational Medicine, Kavli Neuroscience Discovery Institute, Johns Hopkins University, 3400 N. Charles St Baltimore, MD, 21218, USA.

* Corresponding Author: Ting.Xu@childmind.org

Abstract

Compelling evidence suggests the need for more data per individual to reliably map the functional organization of the human connectome. As the notion that 'more data is better' emerges as a golden rule for functional connectomics, researchers find themselves grappling with the challenges of how to obtain the desired amounts of data per participant in a practical manner, particularly for retrospective data aggregation. Increasingly, the aggregation of data across all fMRI scans available for an individual is being viewed as a solution, regardless of scan condition (e.g., rest, task, movie). A number of open questions exist regarding the aggregation process and the impact of different decisions on the reliability of resultant aggregate data. We leveraged the availability of highly sampled test-retest datasets to systematically examine the impact of data aggregation strategies on the reliability of whole-brain functional connectomics. Specifically, we compared functional connectivity estimates derived after concatenating from: 1) multiple scans under the same state, 2) multiple scans under different states (i.e. hybrid or general functional connectivity), and 3) subsets of one long scan. We also varied connectivity processing (i.e. global signal regression, ICA-FIX, and task regression) and estimation procedures. When the total number of time points is equal, and the scan state held constant, concatenating multiple shorter scans had a clear advantage over a single long scan. However, this was not necessarily true when concatenating across different fMRI states (i.e. task conditions), where the reliability from the aggregate data varied across states. Concatenating fewer numbers of states that are more reliable tends to yield higher reliability. Our findings provide an overview of multiple dependencies of data concatenation that should be considered to optimize reliability in analysis of functional connectivity data.

INTRODUCTION:

Functional connectomics is a mainstream modality for mapping brain organization (Greicius et al., 2003; Power et al., 2014; Smith et al., 2013; Sporns, 2013; Yeo et al., 2011). Initially focused on the demonstration of findings at the population-level, the past decade has witnessed a burgeoning literature focused on the delineation of differences among individuals and clinical groups (Braga and Buckner, 2017; Fornito and Bullmore, 2015; Laumann et al., 2015). Recognizing concerns about reproducibility stemming from a reliance on small samples, researchers have raised the bar for sample size, leveraging the growing availability of public datasets to achieve this goal, for example, Human Connectome Project, UK Biobank, 1000 Functional Connectomes, Consortium for Reliability and Reproducibility, etc. (Biobank, 2014; Biswal et al., 2010; Van Essen et al., 2013; X. N. Zuo et al., 2014). Unfortunately, the sample size is not the sole consideration for efforts to achieve reproducible findings in studies of individual and group-differences. The reliability of the measures obtained directly impacts the sample sizes required and the likelihood of replication (Matheson, 2019; Zuo et al., 2019). Recognizing this reality, researchers are increasingly emphasizing the need to obtain larger amounts of data per individual, as reliability appears to be directly related (Birn et al., 2013; Gordon et al., 2015; Noble et al., 2017; Xu et al., 2016).

While the need for more data per individual appears to be straightforward, how to achieve the desired amount of data is not. It is not always feasible to obtain more data due to practical limitations of a crowded scan protocol, or tolerability of the scanning environment (Krause et al., 2019; Meissner et al., 2020; Menon et al., 1997). Additionally, this solution does little to address questions about how to improve the amount of data available for analysis in existing data acquisitions. In response, a growing theme in the literature suggests that fMRI data from different fMRI scan states (e.g., rest, task, movie) can be combined to achieve the desired quantities (Elliott et al., 2019; O'Connor et al., 2017; Schmälzle et al., 2017). At present, there is limited guidance about the relative trade-offs of using concatenated data, or how to best do so.

In this study, we examine the impact of data concatenation strategies on the reliability of functional connectomics and differences that can arise from the specific concatenation method employed. First, we examine the impact of concatenating data from multiple short scans versus a single long scan. This is an important issue in the literature, as studies focused on hyperkinetic populations, such as the Adolescent Brain Cognitive Development (ABCD) study by National Institutes of Health (NIH), have advocated for using multiple shorter scans as a means of improving tolerability and compliance (i.e., low head motion) (Casey et al., 2018). Second, we examine the impact of concatenating data from different states versus the same state. A recent study suggested that the calculation of functional connectivity from multiple states yields data that has superior reliability to that from the same state (Elliott et al., 2019). In this work, they compared a hybrid dataset, generated by concatenating data from different scans versus resting state data. One question that

arises is if the observed advantage was truly the product of combining different states, versus the concatenation of small segments of data from different scans - which was shown to be advantageous (relative to fewer large segments) in the single-subject MyConnectome dataset (Laumann et al., 2015). Third, we address the question of whether there is any advantage to first calculating connectivity matrices for each scan and then combining, or to concatenating time-series data and then calculating connectivity. To date, there is little guidance in the literature regarding this issue. Finally, we examine the impact of the number of test-retest units versus the amount of data per unit on test-retest reliability as well as how concatenation of smaller segments of data contributes to different combinations of numbers of test-retest units and length of each subset (Noble et al., 2017).

It is important to clarify that the goal of the present work is not to question the value of combining all available data in a given study to optimize reliability for a given collection, as that is obvious from the existing literature (Elliott et al., 2019; Noble et al., 2019, 2017; Xu et al., 2016). Instead, our goals are twofold. First, to address the issue of data concatenation and how to understand the trade-offs of different decisions when designing a new experiment for acquisition of a fixed amount of data. Second, to clarify potential confusions in the literature regarding determinants of reliability - most notably, the reported advantages for hybrid (i.e., mixed state) functional connectivity measures, and the relative trade-offs related to the number of sessions versus scan duration (Elliott et al., 2019; Noble et al., 2017).

METHODS:

All analyses in the present work were carried out using publicly available datasets selected based on the inclusion of extensive test-retests fMRI.

Human Connectome Project (HCP). We made use of the HCP S1200 release, which includes resting and task fMRI data from 217 (104 male, age=28.5 +/- 3.7 years) unrelated participants (Glasser et al., 2013; Marcus et al., 2013). Extensive descriptions of the data and the minimal preprocessing applied can be found in prior publications (e.g., Glasser et al., 2013; Marcus et al., 2013). In brief, for each participant, the dataset includes 4 resting fMRI (rfMRI) scans obtained across two days - namely REST1_LR, REST1_RL, REST2_LR and REST2_RL in HCP files. Here the LR and RL represent left-to-right and right-to-left phase coding directions that were used in the gradient-echo EPI sequence (TR=0.72s, TE=33.1ms, flip angle=52°, FOV=208x180mm, resolution=2x2x2mm); each rfMRI scan contains 1200 volumes (~15 mins). To control for the effects of head motion, we further selected a subsample from the HCP dataset as a low-motion replication dataset. Specifically, we selected participants with 'clean' rfMRI data after the HCP minimal preprocessing on the Power-'voxplot' (Power et al., 2017). This subsample consists of 22 subjects selected by visual inspection (subID in Supplementary Table 1).

HCP test-retest dataset. We also used the HCP test-retest dataset, which contains 7 tasks and 2 resting-state sessions, repeated twice per participant. Six tasks were used in our analyses including working memory (WM, 405 volumes), gambling (GAM, 253 volumes), motor tasks (MOT, 284 volumes), which were collected during the first day, and language (LAN, 316 volumes), social (SOC, 274 volumes) and relational (REL, 232 volumes) tasks collected on the second day (Glasser et al., 2013; Van Essen et al., 2013). The emotion task (176 volumes) was removed in the analyses because its minimal amount of volumes did not meet the low-motion criteria (details in study-2 section). For each task, there were two runs (one with LR phase coding direction and the other with RL). Thirty-one participants who have completed all the tasks and resting scans with low head-motion (mean FD < 0.25) were included in our analyses.

HNU dataset. The Hangzhou Normal University (HNU) dataset is openly available via the Consortium of Reliability and Reproducibility (CoRR: http://fcon_1000.projects.nitrc.org/indi/CoRR/html/hnu_1.html) (X.-N. Zuo et al., 2014). The dataset includes 300 scan sessions from 30 participants (15 males, age=24 +/- 2.41 years) who were scanned for 10 sessions over a month. Each session included an rfMRI scan acquired at the same GE MR750 3T scanner using a T2*weighted EPI sequence (TR=2000ms, TE=30ms, flip angle=90°, resolution=3.4x3.4x3.4mm, FOV=220mm2, 300 volumes, 10 mins). The details of this dataset were described in prior studies (Chen et al., 2015). We selected this dataset because the time duration between retest datasets is equally controlled across participants (3 days duration between two retest sessions) and the head motion was relatively low (mean framewise displacement [mean-FD] < 0.2mm for each of 300 scans, less than 1% [n=3] of timepoints within each scan has FD >0.2mm).

MSC Dataset. The Midnight Scan Club (MSC) dataset consists of 10 participants, whom each participated in 10 fMRI sessions over ten days beginning at midnight (https://openneuro.org/datasets/ds000224) (Gordon et al., 2017). Each session included 30 mins of resting fMRI using a gradient-echo EPI sequence (TR=2200ms, TE=27ms, flip angle=90°, resolution=4x4x4mm, 36 slices, 818 volumes). Consistent with the previous study, one participant with high head motion was excluded in the current work. The details of the imaging acquisition are described in the previous studies (Gordon et al., 2017; Gratton et al., 2018). Instead of using the temporal mask (FD<0.2mm) provided with the preprocessed data, we opted for a slightly less conservative threshold (FD<0.3mm) for further censoring high-motion time points to control the head motion while ensuring enough time points remained per scan (> 300TR).

Data Preprocessing

HCP and HCP test-retest datasets. We used the publicly available version of the dataset that has been processed with the HCP minimal preprocessing pipeline (Glasser et al., 2013). In line with prior resting state studies, nuisance regression and bandpass filtering (0.01-0.1Hz) were then applied (Elliott et al., 2019). The nuisance regressors included Friston's 24 head motion parameters, mean signals from white matter (WM) and cerebrospinal fluid (CSF), and linear and

quadratic trends. The impact of regression with and without global signal was tested in our analyses. Given our focus on functional connectivity, nuisance regression and bandpass filtering (0.01-0.1Hz) were carried out for minimal preprocessed data from task conditions. In addition, we examined the impact of task-evoked signals on our findings by adding regressors to account for task events/stimuli (Fair et al., 2007). Finally, the preprocessed data were projected to the cortical surface and smoothed with FWHM=6mm along the surface.

MSC. We made use of the preprocessed version of the MSC that is publicly available on OpenfMRI (https://www.openfmri.org/dataset/ds000224/) (Gordon et al., 2017; Gratton et al., 2018). The preprocessing steps included for this data included slice timing correction, grand mean scaling, and motion correction. The fMRI data were co-registered to the first session for distortion correction followed by detrending, nuisance regression (Friston's 24 motion parameters, WM, CSF, and global signal) and bandpass filtering (0.009-0.08Hz). The details of the preprocessing steps were described in Gordon et al. (2017).

HNU. The HNU dataset was preprocessed using the Connectome Computation System (CCS: http://lfcd.psych.ac.cn/ccs.html) (Xu et al., 2015), a functional connectivity-focused end-to-end analytic pipeline. Briefly, preprocessing steps for functional data using the CCS included: removal of the first 5 TR's, despiking, motion correction, grand mean scaling, Friston 24-parameter model nuisance regression and bandpass filtering (0.01-0.1Hz). The preprocessed fMRI data were co-registered to anatomical image and projected to the native midthickness surface and smoothed with FWHM=6mm along the surface.

Functional Connectivity and Networks

To calculate functional connectivity matrices for each participant, vertex-wise time-series were first averaged within each of the 360 regions using a recent multi-modal parcellation atlas (Glasser et al., 2016). Pairwise Pearson correlations were calculated to generate a 360 x 360 parcel-to-parcel connectivity matrix. Reliability was calculated for each functional connection in the upper triangle of connectivity matrices (64620 connectivities). Yeo-Krienen 7 Networks was used to cluster the parcel-wise connectivity into large-scale networks (visual, somatomotor, dorsal and ventral attention, limbic, frontoparietal, and default) (Yeo et al., 2011). The network identity was assigned to each parcel using the winner-take-all approach based on parcel-to-network overlap (i.e. percentage of parcels covered by the network).

Test-retest reliability Analyses

Terminology. To avoid a possible misunderstanding of terms used in the following section, we first clarify four key terms here: 1) *Scan* - a contiguous unit of fMRI data, defined by the start and stop of the MRI scanner. 2) *Session* - a unit of time that contains either a single or series of MRI experiments, defined by the participant entering and exiting the MRI scanner. 3) *Segment* - an epoch of contiguous fMRI time-series that is cut from a scan for data concatenation over more scans or sessions. 4) *Subset* - in the current study, since the test-retest dataset for reliability

calculation are not necessarily acquired from a single scan or session, we define each of the test and retest datasets as a subset regardless of whether the data were from a contiguous scan or concatenated from multiple scans. As commonly performed in the literature, z-score normalization was conducted for each of the segments before concatenation.

Intra-class correlation (ICC). Intra-class correlation was calculated to estimate test-retest reliability using Linear Mixed Model (LMM) for functional connectivity (O'Connor et al., 2017; Xu et al., 2016). For a given connection c denoted as $Y_{ij}(c)$, i represents the participant and j indicates the test and retest subset. Age, gender, global mean for functional connectivity, and head motion were included in the model as covariates.

$$Y_{ij}(c) = \mu_{00}(c) + \gamma_{i0}(c) + age_i + sex_i + G_{ij} + meanFD_{ij} + \epsilon_{ij}(c).$$

The intercept $\mu_{00}(c)$ in the model represents the fixed effect of group average at connectivity c, while $\gamma_{i0}(c)$ represents the random effect for *i*th participant. We also included age, sex, global mean for functional connectivity (G_{ij}), and mean FD as covariates in the model. The inter-individual variance σ_γ^2 of the random effect and the variance σ_ϵ^2 of residual ϵ_{ij} were estimated using the restricted maximum likelihood (ReML) method in R (http://cran.r-project.org/web/packages/nlme). ICC was calculated by dividing the inter-individual variation σ_γ^2 by the sum of σ_γ^2 and residual variance σ_ϵ^2.

General study flow. In this study, we examined the impacts of data aggregation on the reliability of functional connectivity from different data types (i.e. resting, task, hybrid), and concatenation methods. Figure 1 illustrates the specific comparisons of data aggregation strategies. More detailed descriptions for each study are introduced in the following sections.

1
2 **Figure1. Graphical summary of comparisons for different data aggregation strategies.**
3
4 *Study-1. Concatenating from multiple scans versus a single long scan.*
5
In order to address whether the protocol that required multiple shorter resting scans rather than a
single scan could achieve comparable or higher reliable functional connectomics, we first
examined the reliability of concatenating data from multiple scans versus that from a single long
scan. Three datasets with multiple scans separated by a regular time interval between retest
sessions were used in this analysis: 1) the *HCP* (n=217), which included 2 sessions per participant
(2 R-fMRI scans per session; 1 day apart between two sessions), 2) the *HNU* (n=30), which

included 10 R-fMRI scans per participant (3 days apart between two sequent sessions), and 3) the *MSC* (n=9) with 10 R-fMRI scans per participant (1 day apart between two sequent sessions). Of note, to maintain the continuity of R-fMRI scans, we performed the above analyses on the uncensored dataset and replicated this in the low-motion subsample of HCP dataset as well.

For the HCP dataset, we calculated the reliability of contiguous data across sessions (i.e. between Day 1 and Day 2), specifically, between Day 1 LR and Day 2 LR scans, and between the Day 1 RL and Day 2 RL. For the concatenated data, we used two resting fMRI scans (LR and RL, 600 TRs per scan) collected in Day 1 as the data pool to extract time-series segments and concatenate into subset 1. Similarly, data segments selected from two scans (LR and RL) in Day 2 were concatenated into subset 2.

Of note, the used scans matched on sequence (i.e. only LR or only RL) for contiguous data represents the test and retest of 15 mins scans (1200 TRs) with the same phase coding sequence for calculation of test-retest to obtain the best-case scenario for the reliability of contiguous data. An obvious concern that can arise is that the concatenated data combines across phase-encoding directions, while the contiguous data did not. To address this concern, we also calculated reliability for the scenario where they are not matched to estimate the worst case direction over a day (Fig. S1A).

In the HNU dataset that consists of 10 sessions per participant, sequential sessions were used as test-retest subsets (i.e. test-retest between session #1 and #2, #2 and #3, …, #9 and #10) to examine the reliability of contiguous scans (280 TRs, ~ 10 mins). For the concatenated data, we first split 10 sessions into two data pools to generate test and retest subsets. Specifically, we used the first five scans (i.e. sessions 1-5) as the data pool to generate concatenated data for subset 1 and the last five scans (i.e. sessions 6-10) for subset 2. Similarly, different combinations of numbers of segments and lengths of segments to generate concatenated data were applied (i.e. 2 segments x 140 TRs, 4 segments x 70 TRs, 8 segments x 35 TRs). For the concatenated subset with 2 or 4 segments, each segment was randomly selected from a single scan to guarantee the concatenated data were merged from different scans. To ensure no contiguous segments in a single scan were selected in creating a concatenated subset with 8 segments, we randomly selected four scans from the data pool and then randomly selected segments from half of each selected scan to generate 8 segments into a subset.

In the MSC dataset, which contains 10 scan sessions per participant, a procedure similar to that applied in the HNU dataset was carried out to yield test-retest subsets. In short, the reliability was examined for contiguous data between two sequential sessions (800 TRs, ~ 30-mins per session), as well as concatenated data from different combinations (i.e. 2 segments x 400 TRs , 4 segments x 200 TRs, 8 segments x 100 TRs, 16 segments x 50 TRs, 800TRs [30 min] in total per subset).

Study-2. Concatenating from different states versus the same state.

A recent study suggested that functional connectivity calculated by concatenating multiple fMRI task scans in the HCP dataset exhibits higher test-retest reliability than that from an equivalent amount of pure resting state fMRI data (Elliott et al., 2019). While this may be true, prior work using the MyConnectome dataset highlighted the advantage of concatenation from shorter scans over a single scan (Laumann et al., 2015). As such, it is not clear whether the better reliability for merged data from different states (referred to here as the 'hybrid' condition) is driven by the concatenation advantage or the combination of experiment states. To address this question, we generated the concatenated resting subsets that were matched to the hybrid condition with respect to the number/length of segments and compared the reliability between hybrid and concatenated resting data. In addition, we further examined the impact of concatenation from combinations of task states.

Concatenated task versus concatenated resting state. We first evaluated the reliability of concatenated data over available scans (2 scans, LR and RL, 5.6 min in total) from the same task only versus resting state (2 scans, LR and RL, 5.6 min in total). We also compared the reliability of hybrid data yielded from two different fMRI tasks as compared to the concatenated data from a single state (task or resting). The reliability of six task states, resting state, as well as the hybrid from two different tasks was calculated. The effects of global signal regression (GSR) and task regression were examined in our analyses. Of note, we used the resting without ICA-FIX, consistent with the preprocessing procedure of task data. We also tested the ICA-FIX resting data in the supplementary materials (Fig. 7, S5).

Hybrid versus concatenating from resting state. We made use of the HCP test-retest dataset to assess the reliability of hybrid versus resting-state conditions between test and retest measurements. Specifically, we used six tasks to generate all of the possible hybrid subset combinations with regard to task state and encoding direction (LR and RL), consisting of 2 different tasks (2 tasks x 232 volumes, 5.6 min), 2 different task that each contains 2 scans (2 tasks x 2 scans x 232 volumes, 11.1min), 4 different tasks (4 tasks x 232 volumes, 11.1min) and 6 different tasks (6 tasks x 200 volumes, 15 min). To match the hybrid data, concatenated resting-state subsets for comparisons were created by concatenating 2, 4, and 6 segments. The segments were contiguous volumes (i.e., the first 232 or 200 volumes) from different resting scans, except for the 6-segments combination in which two additional segments were selected (#601-800 volumes) since only 4 resting scans were acquired. In addition, we compared the reliability of concatenated hybrid and resting connectivity against that from a single contiguous resting scan truncated to the same time duration.

Study-3. Calculate and then combine versus Combine and then Calculate.
When multiple scans are acquired, apart from combining time-series first, we can also calculate the functional connectivity per scan then average the connectivity afterwards. In this section, we have tested whether one strategy is superior to the other using the HCP and HNU datasets.

In the HCP dataset, resting fMRI data from Day 1 LR and RL scans were used for 1 subset while Day 2 LR and RL scans were used for the 2nd subset. Reliability was tested between the Day 1 subset and Day 2 subset. The functional connectivity matrix for each subset was either calculated from concatenated data over LR and RL scans, or averaged from connectivity that calculated from each of LR and RL scans separately. We tested 3 different time lengths, 1) 5 minutes by 2 scans per subset, 2) 10 minutes by 2 scans per subset, and 3) 15 minutes by 2 scans per subset.

In the HNU dataset, we selected two scans (session #1-2) to create subset 1 while two scans (session #6-7) for subset 2. In this way, the time duration between test-retest subsets are fixed to 12 days (scanned once every 3 days). Functional connectivity was calculated in both strategies from two sessions per subset. Similarly, we tested 2 different time lengths, 1) 5 minutes by 2 sessions per subset, and 2) 10 minutes by 2 sessions per subset.

Study-4. More test-retest subsets versus more amount of data per subset.
Beyond the general rule of 'the more the better' in data collection, in this section, we focused on how test-retest reliability increases with more numbers of subsets versus more amount of data per subset. We examined the reliability for different combinations of these two factors.

Test-retest subsets with concatenation. The MSC dataset was used here as it contains 10 sessions x 30 mins data per subject. We tested the number of subsets varied from 2, 3, 4, 5, and 6; the amount of time per subset varied from 10, 12.5, 15, 17.5, 20, 22.5, 25, 30, 35, 40, 50, and 60 mins. For a combination of k subsets and t *minutes* per subset, the subset data was concatenated from x numbers of short contiguous segments (2.5 mins per segment, $x=t/2.5$). Specifically, for each participant, we first randomly cut all available data into a few 2.5 mins (68 volumes) segments as a segment pool. We then randomly selected $k*x$ segments to create k subsets. The test-retest reliability was calculated for all combinations of numbers of subsets and the amount of data per subset. We replicated the analyses in the HCP dataset for different combinations of 2, 3, 4, 5 subsets by 10, 12.5, 15, 17.5, 20, 22.5, 25 mins of data per subset. The subsets were concatenated in a similar way from short segments (2.5 mins, 208 volumes).

Test-retest subsets without concatenation. We also considered the test-retest subset acquired naturally in a single fMRI session instead of concatenated from multiple shorter scans in the MSC dataset. Similarly, we tested the number of subsets varied from 2, 3, 4, 5, and 6, while the amount of time per subset varied from 10, 12.5, 15, 17.5, 20, 22.5, 25, and 30 mins. For a combination of k subsets and t *minutes* of scan duration, k sessions ($k=2,3,..,6$) were randomly selected k sessions first and t min of contiguous time points from each of selected k sessions. The test-retest reliability was calculated for all combinations of numbers of sessions and scan duration.

RESULTS:

Study-1. Concatenating from multiple scans versus one long scan. Here, we compared the ICC distribution for edge-wise functional connectivities based on fMRI data concatenated from multiple scans, with that obtained from a single long scan. Generally, using the HCP data, we found that when the amount of data was equated, there was a clear advantage for multiple scans from the perspective of edgewise reliability. Specifically, the concatenated subset (7.5 min from 2 scans) yielded higher ICC's than the contiguous data (15 min from a single scan) (Fig. 2A, ICC matrices in Fig S1B). The significance of our findings did not dependent on whether GSR was included in preprocessing or not (without GSR: $t_{(64619)}=168.14$, $p<0.001$, GSR: $t_{(64619)}=164.35$, $p<0.001$, paired t-test). Such advantages of concatenation were observed across all networks (Fig. 2B). Similar findings were obtained in the HNU (contiguous scan duration = 10 minutes, Fig. 2C-D) and MSC datasets (contiguous scan duration = 30 minutes, Fig. 2E-F), as well as the low-motion HCP subsample - all achieving statistical significance (Fig. S2, left panel).

With regard to the concatenation window size, we found that from a reliability perspective, a higher number of shorter fMRI data segments appeared to engender advantages over a smaller number of larger segments. In the HNU dataset, 10 min of a contiguous scan yielded 12% of connections with good reliability (ICC>=0.6), which increased to 26% for 8 X 1.25 min segments from four sessions. In the MSC dataset with 30 min of data, shorter segments consistently showed higher ICC than contiguous data (contiguous: 24% of connectivities were good; 16 X 1.875 min segments: 41% good). Of note, this advantage does not appear to result from the process of Z-scoring (i.e., mean centering and variance normalization) segments prior to combining; there was no advantage, and even slightly worse reliability, observed when segments were selected from the same scan (Fig. S1C). We also tested whether concatenating time-series data from the onset of each scan could achieve higher reliability, but did not find any clear evidence there is the onset effect (Fig. S2, right panel).

Figure 2. **Edgewise functional connectivity calculated from concatenated scans is more reliable than that based on a single contiguous scan of equal length**. **(A)** Empirical cumulative distribution and bar plots of mean intraclass correlation coefficient (ICC) with error bars (standard deviation) for test-retest reliability of functional connectivities from contiguous and concatenated resting-state fMRI scans; results for calculation based on data with and without global signal regression (GSR) are depicted. **(B)** Empirical cumulative distribution of ICC for each network. Distribution of ICC from contiguous data is shown in grey while colored lines represent ICC from concatenated data. See FC and ICC matrices in Fig S1B. **(C)** Empirical cumulative distribution of ICC and **(D)** stacked bar plots depicting proportion of connections with poor, moderate, good and excellent ICC for contiguous and concatenated resting-state scans, calculated using the HNU dataset and the Midnight Scan Club dataset **(E, F)**.

Study-2. Concatenating from different states versus the same state. Study-1 showed that the concatenation of data from multiple scans yielded connectivity estimates with higher reliability than those obtained using a single scan. However, the data was all obtained during the resting state. Here, we take the next logical step, and examine: 1) the reliability of concatenated data from a task state versus resting state, 2) the reliability of concatenated data from different tasks versus the same task, and 3) whether the benefits of concatenation are maintained when concatenating data from multiple states (i.e. hybrid) versus a single state.

i) Concatenated task versus concatenated resting state. Using HCP test-retest dataset, we concatenated the available task scans (232 volumes x 2 scans, 5.6min in total) for each task state and compared their reliabilities to the concatenated resting data (232 volumes x 2 scans), as well as the contiguous resting data (464 volumes from a single scan). We found that when task regression was performed, edgewise functional connectivities for two of the task states (i.e.,

language and social) exhibited higher ICC's than those from either concatenated or contiguous resting data. When task regression was not applied, reliability scores for edgewise connectivities increased for all six task states, becoming higher than those from resting state (Fig. 3A). Similar findings were observed when GSR was carried out (Fig. S3).

ii) Hybrid versus task state. Next, we considered data concatenated from 2 different tasks, instead of 2 scans from the same task. We systematically tested all the possible combinations of concatenating 2 different tasks. In general, data concatenated from the same task yielded higher reliabilities than that generated from possible combinations of different tasks (i.e. hybrid) (Fig. 3B). It is important to note that hybrid data generated from two states associated with more reliable states (e.g., language and social tasks) tended to yield greater reliabilities than the other possibilities (e.g., motor and working memory tasks).

Figure 3. Reliability of edgewise functional connectivity measures calculated using each resting-state, task and hybrid fMRI data. (A) Proportion of connections with poor, moderate, good and excellent ICC when calculated for resting state and each of six task conditions in the HCP dataset, with (left-panel) and without task regression (right-panel). **(B)** Mean ICC for functional connectivity measures based on hybrid data generated by concatenating two scans from two different task states (off-diagonal) and the same task state (diagonal). See results with GSR in Fig. S3.

iii) Hybrid versus resting state. We further compared the reliability of edgewise connectivities from multiple task fMRI scan types (i.e. hybrid) to those from resting fMRI data, concatenated from multiple scans, as well as from equal amounts of resting data from a single scan. Besides the combination of 2 task states (2 scans, 5.6 min in total) that were tested above, we also tested the hybrid connectivity of 2 task states generated from a higher number of scan types (4 scans, 11.1 min in total). The concatenated resting data (equal length) were generated from 2 and 4 resting scans respectively, as well as equivalent length of contiguous resting data truncated from a single scan (Fig. 4). As expected, more data was better, regardless of hybrid or resting state. Concatenated resting data exhibited higher reliabilities than half of the 15 possible hybrid combinations from 2 task scans with task regression. When compared with hybrid from 4 scans, the concatenated resting data yielded the second-highest reliabilities compared to other hybrid combinations, except for the hybrid generated from language and social tasks (Fig. 4). In contrast, when task regression was not performed, the hybrid data showed generally higher reliabilities than concatenated and contiguous resting data. Similar trends were found for GSR preprocessed data as well (Fig. S4).

Figure 4. Reliability of edgewise functional connectivity measures calculated for resting and hybrid data generated from 2 tasks using either 2 or 4 segments. The label color for task states from cold to warm represents the reliability (i.e., mean ICC) of each state from low to high (detailed distribution shown in Fig. 3A). The same length of contiguous resting data was truncated from LR and RL scans of the Day 1 session (red dot: 5.6 min, RL>LR; red square: 11.1 min, RL>LR). The concatenated resting data was generated from 2 scans (blue dot: 5.6 min, LR and RL scans from Day 1) and 4 scans (blue square: 11.1 min, LR, RL scans from Day 1 and Day 2). See results with GSR in Fig. S4.

Besides the combinations of 2 task states we tested above, we also used 4 and 6 task states to generate different lengths of hybrid data, and systematically tested all possible combinations of different tasks (details in Method). We found that compared with contiguous resting data, that hybrid data generated from 2 tasks (total data: 5.6 min), 4 tasks (11.1 min), or 6 tasks (15 min) did not necessarily exhibit higher reliabilities (Fig. 5 with task-regression, Fig. S5 without task-

regression). When task-evoked activation was regressed out, ten out of thirty combinations of the shorter, two-task hybrid had an advantage over the resting-state with respect to reliability (Fig. 5, left panel). With more data (hybrid: 4 different tasks and 6 different tasks, resting: 4 segments, 6 segments), the concatenated resting data that matched with hybrid concatenation segments showed a clear advantage over all hybrid conditions and contiguous resting as well (Fig. 5, middle and right panels). Similar findings were observed in data with GSR (Fig. 5, gray line). When matching the concatenation strategy for resting conditions, the concatenated resting data offered higher reliability than most of the hybrid combinations from different task states (Fig. 5, gray triangles on the blue lines).

Figure 5. Reliability of edgewise functional connectivity for resting and hybrid data as a function of the numbers of task states combined in the concatenation process (2, 4 and 6 different tasks). The same length of contiguous resting data was truncated from LR and RL scans of Day 1 session (highlighted with red lines). The concatenated resting data was generated from 2, 4, and 6 segments of resting scans (highlighted with blue lines). See results without task regression in Fig. S5.

We also assessed the ICC of hybrid conditions from task scans without task regression. As depicted in Fig. S5, connectivity reliabilities for hybrid task scans were higher without task regression than with. When comparing such hybrid conditions with contiguous resting data, the hybrid conditions consistently yielded higher ICC's than contiguous resting data (Fig. S5). The concatenated resting data, on the other hand, showed increased ICC and became more likely to have higher reliabilties than hybrid combinations from more than 2 states (i.e. 4 tasks and 6 tasks). A similar trend was observed with GSR data (Fig. S5, gray line).

iv) Hybrid with more task states versus hybrid with fewer task states.
We previously noted that connectivity reliabilities from the resting state were not superior to those from all of the task states (Fig. 3A). It seemed that combining more different task states (>=4 tasks) might have a negative impact on reliability, resulting in lower reliabilities than resting state. Thus, we further controlled the number of segments and varied the number of task states combined.

Specifically, we compared the reliabilities yielded from hybrid data concatenated from 4 different
tasks (4 scans) as we examined above versus 2 different tasks (2 scans per task, 4 scans in total).
As we expected (Fig. 6, dark green diamonds), hybrid combinations from fewer states (2 tasks)
appeared to yield higher reliabilities than hybrid from 4 tasks. In particular, hybrid data generated
from language and social tasks exhibited higher reliabilities than concatenated resting data. Of
note, language and social tasks are also the most reliable tasks and showed higher reliability than
resting state (Fig. 3A). These findings also suggest that data concatenated from reliable states tend
to yield more reliable connectivities. Similar observations were found in data with GSR (Fig. 6,
gray line, light green diamonds).

Hybrid with more task states versus fewer task states

10
11 **Figure 6. Reliability of edgewise functional connectivity for hybrid data as a function of the**
12 **numbers of task states (2 versus 4 tasks) combined in the concatenation process.** Hybrid

1 combinations with less task states (green: 2 tasks) exhibited higher reliability than hybrid
2 combining from more task states (black: 4 tasks).
3
In addition, we also examined reliabilities for resting data that ICA-FIX was applied to in HCP
minimal preprocessing pipeline and compared with task and hybrid conditions. First, we measured
the similarity (Pearson's *r*) of functional connectivity patterns within individuals under different
preprocessing options across task, resting and hybrid conditions. We found that the GSR option
dominated the functional connectivity patterns for resting, task as well as hybrid data (Fig. 7A).
The group averaged functional connectivity with different preprocessing (i.e. GSR, ICA-FIX, task-
regression) is shown in Fig. 7C. It is worth noting an interaction between ICA-FIX and GSR (Fig.
7B). Without ICA-FIX, no GSR option provided a higher ICC than GSR (contiguous: $t_{(64619)}$=-
26.187, *p*<10-150; concatenated: $t_{(64619)}$=-35.101, *p*<10-267), while GSR showed an advantage
over no GSR when ICA-FIX was performed (contiguous: $t_{(64619)}$=57.873, *p=0*; concatenated:
$t_{(64619)}$=40.871, *p*=0). When compared to hybrid, resting conditions with GSR and ICA-FIX
exhibited higher ICC than most of the hybrid combinations (Fig. S5, "X" marks in grey color).
16

17
18 **Figure 7. Effect of preprocessing steps on similarity of functional connectivity and reliability.**
19 **(A)** Averaged within-individual similarity (Pearson's *r*) of functional connectivity patterns for rest,
20 task, and hybrid data (5.6 min in total) with different preprocessing options. Working memory

(WM) state was shown as an example of the task condition and concatenation from GAM and LAN for the hybrid condition. **(B)** Proportion of connections with moderate, good and excellent ICC for contiguous and concatenated resting-state data preprocessed with and without both GSR and ICA-FIX. **(C)** Group averaged functional connectivity matrices with different preprocessing options.

Study-3 Calculate and then combine versus combine and then calculate. Besides time series concatenation, another data aggregation strategy is to first calculate the functional connectivity, then average connectivity matrices across scans. Here, we further compared these two strategies using the HCP dataset. We have included two scans, each scan varied from 5 min, 10 min, and 15 min for data combination. The strategy of concatenating the time-series first was denoted as Strategy-T, while calculating the FC per scan then averaging the FC was denoted as Strategy-A. We found no significant difference between Strategy-T and Strategy-A for 5 min and 15 min data (Fig. 8). A slightly better ICC was detected for 10 min ($t_{(64619)}$=2.59, p=0.001) for Strategy-T. Given the large number of the degrees of freedom in the t-test and the edges (connectivities) were not independent from one another, we considered no clear evidence that one strategy is superior to the other and deem the two strategies equivalent in practice. Similar findings were replicated in the HCP low-motion subsample and the HNU dataset (Fig. S6).

Figure 8. Calculation of edgewise functional connectivity measures for scans individually and then averaging, versus calculation after concatenation of scans. Two segments of 5 min, 10 min, and 15 min of data were generated. The strategy calculating the FC of each segment first then average all the FC as the final FC for each subset was denoted as Strategy-A, while concatenating time-series of all segments then calculating FC per subset as Strategy-T. The stacked bar and the empirical cumulative distribution of ICC showed no differences in ICC distribution between two strategies. The scatter plot shows the ICC of functional connectivity was almost the same between two strategies for 10 min data (2 segments x 5 min).

Study-4. Delineating the trade-off of amount of data per subset and number of subsets in evaluations of reliability. In Study 1, we showed that more data per subset improved the reliability between two subsets, regardless of whether the subset was contiguous or concatenated data. These findings echoed the general rule of 'the more the better' in data collection. Here we address a confusion that may arise in evaluations of reliability - whether increasing the number of subsets improves reliability more quickly than increasing amounts of data per subset.

We first focused on the contiguous data using the MSC dataset (30 min x 10 sessions per subject). We tested subsets generated from a single scan of 10, 12.5, 15, 17.5, 20, 22.5, 25, 30 min data, while the number of subsets was increased from 2 to 6 subsets. As shown in Fig. 9A, we observed that the reliability increased more quickly with increasing amounts of data per subset compared to increasing the number of subsets. We also tested the reliability for each subset created by concatenating smaller time-series segments (2.5 min) randomly selected within the subject from all available data without replacement (Fig. 9B). Similarly, when the total amount of the data was used, more data assigned to subsets yielded higher reliability than when the data was split into more subsets. Yet, increasing the number of subsets appeared to have fewer decreases in the reliability estimation (Fig. 9B). Overall, when multiple scans were acquired, concatenating multiple scans into two subsets, instead of treating them as multiple scans obtained higher ICC estimations.

Figure 9. Reliability of functional connectivity estimated across different numbers of subsets and different length of data within each subset. Bubbles represent the ratio of ICC values > 0.5 at each combination of the number of test-retest subsets (x-axis) by the duration for each subset (y-axis). The contour line of total amount of time (subsets x duration) are plotted in gray lines. (A) Each subset data was created from a contiguous scan while each subset in (B) was created from concatenation of shorter segments from multiple scans. Two example combinations are marked by rectangles (solid line: 2 subsets with 15 min data per subset, dashed line: 3 subsets with 10 min data per subset).

DISCUSSION:

The present work evaluated the impact of different strategies for combining data from distinct fMRI scans on the reliability of functional connectivity. Several key findings emerged. First, for a given state, we found a clear advantage for combining data from multiple scans of the same state, rather than acquiring an equivalent amount of data from a single long scan. Importantly, we found that this was not necessarily true when concatenation was carried out across different fMRI states (i.e. task conditions), where we observed an advantage for concatenating segments from the same

state rather than different states. When concatenation was performed across differing states, the combination from more reliable states tends to yield higher reliability. We next tested whether there is an advantage for combining time-series data across scans prior to calculating functional connectivity, versus calculating the functional connectivity for each of the individual scans and then averaging; we found no clear evidence of superiority for either strategy. Finally, as a growing number of high characterization test-retest designs are emerging, we drew attention to basic design principles to be considered in the design of test-retest studies.

The present work is not the first to suggest an advantage for concatenation from multiple shorter scans over a single long scan. For example, previous work using the MyConnectome dataset has shown that functional connectivity measurements in a single subject converge faster with multiple scans of shorter length than with a single longer scan (Laumann et al., 2015). One possible reason is that the noise obtained from the scanner (e.g. pink noise or 1/f noise) might be flattened out when concatenating multiple scans together (Afshinpour et al., 2008; Akhrif et al., 2018). When a single long scan is acquired, however, the noise is maintained as the main variation between test and retest sessions, thereby reducing reliability. Another possibility is that the participants might have low head motion at the beginning of each scan (i.e., an onset effect). A recent study found that head motion events occur more frequently with longer scan length and suggested a scanner break inside the scanner to improve head motion in both children and adults samples (Meissner et al., 2020). The present work tested for the presence of an onset effect (i.e., whether concatenating time-series data from the onset of each scan could achieve higher reliability) but did not find any clear evidence to support this hypothesis. This result is consistent with previous findings that the reliability reduced when truncating the time points from the end of the time series (Shah et al., 2016). Nevertheless, the overall results highlight the advantages of concatenation in the calculation of functional connectivity and suggest acquiring multiple shorter scans instead of a single long scan in study design - an approach adopted by the recent NIH ABCD Study (Casey et al., 2018).

It is important to note that the concatenation method itself (i.e. cutting the time-series into shorter contiguous segments and z-scoring the segments) on the same scan did not show any benefits for reliability. This suggests that the non-stationary noise, if any, might not be removed by simply Z-scoring a short contiguous time-series. In fact, our results showed that cutting the original time-series into shorter segments *decreases* reliability (Fig. S1C). These findings indicate the downside of the concatenating shorter scans - a potential loss of the temporal continuity (e.g. auto-correlation) of the fMRI signals, which appear to be important (Arbabshirani et al., 2019; Kumar et al., 2016). One other downside of opting to concatenate multiple shorter scans, rather than pursue a single long scan, is the potential limitations this strategy introduces on temporal dynamic analyses - particularly those focused on the frequency domain (Hutchison et al., 2013). Thus, in the end, it is fair to say that there are benefits to obtaining multiple shorter scans and concatenating them, though the trade-offs should be carefully considered during experimental design.

Aside from the experimental design, our findings suggest that while concatenating scans from multiple scans to maximize data is clearly beneficial, the increases in reliability achieved will be dependent in part by the reliability of the individual scan states being combined. Researchers usually pay attention to the total amount of data merged, yet how the data has been merged might be less heeded. In the current study, we have systematically examined the combinations in generating hybrid data and found that in contrast to prior suggestions, the generation of a hybrid dataset from different states does not necessarily produce functional connectivity measures with higher reliability than those obtained during resting state (Elliott et al., 2019). In our analyses, concatenating resting state with the same concatenation strategy actually showed a substantially higher reliability than most of the hybrid combinations. This could be because merging different states introduces more variations leading to lower reliability. We have examined this hypothesis and found supportive evidence that hybrid data from fewer states are more likely to yield higher reliability than that from more different states. Overall, concatenating data from the same state (i.e., same task scans or only resting scans) showed higher reliability than data combined across states (i.e. hybrid). With the equivalent number of concatenation scans, concatenating from more reliable states trends to yield higher reliability.

Another important finding of the proposed work was the seeming similarity of results when concatenating time-series data prior to calculating the functional connectivity matrix, and the alternative of averaging functional connectivity matrices across independent scans. While the former strategy can be more memory-intensive, the latter is more computationally intensive. Depending on the length of the time-series data per scan, and the number of parcels employed, researchers may prefer to implement one way or the other. Our results suggest that the two methods should yield roughly equivalent functional connectivity matrices. A related question that arises when designing and analyzing highly characterized samples of individuals, is whether to use the maximum amount of data available for the 'test' and 'retest' subsets, which would be split halves of the total data, or to make the individuals scans the test unit and have multiple retest subsets. Our analyses suggest that unless data amounts are more copious than nearly all acquired to date, the aggregation of data into two halves will provide the most reliable test- and retest units (Noble et al., 2017). The alternative approach would provide the tightest confidence intervals for reliability estimation, but as shown in our analyses, the actual reliability will be undesirably low (Zou, 2012).

Finally, the current work examined two preprocessing options that need to be considered in functional connectivity analyses carried out using task fMRI data - global signal regression and task regression. In general, we found that data concatenation impacts are replicable with or without either of these two steps. However, the task and corresponding hybrid data without task regression showed higher reliability than that with task regression. Our finding that reliability was higher for resting state fMRI data than those obtained with any of the six tasks when task-regression was used, makes the impact clear. As previously suggested, task state without task regression does appear to increase the reliability of functional connectivity patterns, possibly by increasing their

stability over time. We also noted that no GSR preprocessing generated higher reliability for task and hybrid data regardless of task regression process. However, it is worth noting the presence of an interaction between GSR and ICA-FIX; the observed advantage for no GSR with resting state data is not observed when ICA-FIX was carried out. When ICA-FIX was performed, functional connectivity from rest with GSR generated higher reliability than without (Parkes et al., 2018).

Summary of Recommendations. Consistent with prior work, the findings of present work reaffirmed the "golden rule": <u>more data is better - whether obtained in a single condition or scan session, or multiple.</u> With that said, our findings allowed us to make a base set of recommendations for consideration in functional connectivity study design and data analysis, when the amount of data available is equal. Specifically, we suggest that when possible, researchers:

1) Acquire and concatenate multiple short scans or sessions, rather than a single long scan. *Caveat:* This recommendation is appropriate for studies focused on static functional connectivity, not dynamic. For the latter, the suitability of multiple scans for analysis is dependent on the specific algorithms employed.
2) Concatenation of data within a single scan condition offers higher reliability than across multiple conditions. Among conditions, concatenating more reliable conditions is more likely to yield higher reliability.
3) After the multiple scans are acquired, the scans should be concatenated into two subsets, instead of treated as multiple.
4) When comparing the reliability, beyond the total amount of data, be cautious with the strategies of how data is concatenated for a fair comparison.

Conclusion:

This work systematically evaluated the impact of data concatenation strategies on test-retest reliability of functional connectivity. When looking at equivalent amounts of data, our results highlight the potential advantages of concatenated data relative to contiguous, and other factors that can lead to higher or lower reliability for concatenated data. We drew attention to dependencies of the resultant reliability of a concatenated scan on the individual scans from which data is aggregated. Finally, we drew attention to the differential impact of preprocessing (i.e. task regression, global signal regression). Combined, the present work provides an overview of multiple decisions that should be considered in efforts to optimize reliability during the acquisition and analysis of functional connectivity data.

ACKNOWLEDGEMENT

This work was supported by gifts from Joseph P. Healey, Phyllis Green, and Randolph Cowen to the Child Mind Institute and the National Institutes of Health (Brain Research through Advancing Innovative Neurotechnologies Initiative Grant Nos. R01-MH111439 [to MPM and Charles E. Schroeder], R24MH114806 [to MPM], and R01MH120482 [to MPM]). Additional grant support for JTV comes from 1R01MH120482-01 (to Theodore D. Satterthwaite, MPM). We thank Russell Takeshi Shinohara and Seok-Jun Hong for valuable discussions and suggestions.

REFERENCES:

Afshinpour, B., Hossein-Zadeh, G.-A., Soltanian-Zadeh, H., 2008. Nonparametric trend estimation in the presence of fractal noise: application to fMRI time-series analysis. J. Neurosci. Methods 171, 340–348.

Akhrif, A., Romanos, M., Domschke, K., Schmitt-Boehrer, A., Neufang, S., 2018. Fractal Analysis of BOLD Time Series in a Network Associated With Waiting Impulsivity. Front. Physiol. 9, 1378.

Arbabshirani, M.R., Preda, A., Vaidya, J.G., Potkin, S.G., Pearlson, G., Voyvodic, J., Mathalon, D., van Erp, T., Michael, A., Kiehl, K.A., Turner, J.A., Calhoun, V.D., 2019. Autoconnectivity: A new perspective on human brain function. J. Neurosci. Methods 323, 68–76.

Biobank, U.K., 2014. About UK Biobank. Available at h ttps://www. ukbiobank. ac. uk/a bout-biobank-uk.

Birn, R.M., Molloy, E.K., Patriat, R., Parker, T., Meier, T.B., Kirk, G.R., Nair, V.A., Meyerand, M.E., Prabhakaran, V., 2013. The effect of scan length on the reliability of resting-state fMRI connectivity estimates. Neuroimage 83, 550–558.

Biswal, B.B., Mennes, M., Zuo, X.-N., Gohel, S., Kelly, C., Smith, S.M., Beckmann, C.F., Adelstein, J.S., Buckner, R.L., Colcombe, S., Dogonowski, A.-M., Ernst, M., Fair, D., Hampson, M., Hoptman, M.J., Hyde, J.S., Kiviniemi, V.J., Kötter, R., Li, S.-J., Lin, C.-P., Lowe, M.J., Mackay, C., Madden, D.J., Madsen, K.H., Margulies, D.S., Mayberg, H.S., McMahon, K., Monk, C.S., Mostofsky, S.H., Nagel, B.J., Pekar, J.J., Peltier, S.J., Petersen, S.E., Riedl, V., Rombouts, S.A.R.B., Rypma, B., Schlaggar, B.L., Schmidt, S., Seidler, R.D., Siegle, G.J., Sorg, C., Teng, G.-J., Veijola, J., Villringer, A., Walter, M., Wang, L., Weng, X.-C., Whitfield-Gabrieli, S., Williamson, P., Windischberger, C., Zang, Y.-F., Zhang, H.-Y., Castellanos, F.X., Milham, M.P., 2010. Toward discovery science of human brain function. Proc. Natl. Acad. Sci. U. S. A. 107, 4734–4739.

Braga, R.M., Buckner, R.L., 2017. Parallel Interdigitated Distributed Networks within the Individual Estimated by Intrinsic Functional Connectivity. Neuron 95, 457–471.e5.

Casey, B.J., Cannonier, T., Conley, M.I., Cohen, A.O., Barch, D.M., Heitzeg, M.M., Soules, M.E., Teslovich, T., Dellarco, D.V., Garavan, H., Orr, C.A., Wager, T.D., Banich, M.T., Speer, N.K., Sutherland, M.T., Riedel, M.C., Dick, A.S., Bjork, J.M., Thomas, K.M., Chaarani, B., Mejia, M.H., Hagler, D.J., Daniela Cornejo, M., Sicat, C.S., Harms, M.P., Dosenbach, N.U.F., Rosenberg, M., Earl, E., Bartsch, H., Watts, R., Polimeni, J.R., Kuperman, J.M., Fair, D.A., Dale, A.M., 2018. The Adolescent Brain Cognitive Development (ABCD) study: Imaging acquisition across 21 sites. Developmental Cognitive Neuroscience. https://doi.org/10.1016/j.dcn.2018.03.001

Chen, B., Xu, T., Zhou, C., Wang, L., Yang, N., Wang, Z., Dong, H.-M., Yang, Z., Zang, Y.-F., Zuo, X.-N., Weng, X.-C., 2015. Individual Variability and Test-Retest Reliability Revealed by Ten Repeated Resting-State Brain Scans over One Month. PLoS One 10, e0144963.

Elliott, M.L., Knodt, A.R., Cooke, M., Kim, M.J., Melzer, T.R., Keenan, R., Ireland, D., Ramrakha, S., Poulton, R., Caspi, A., Moffitt, T.E., Hariri, A.R., 2019. General functional connectivity: Shared features of resting-state and task fMRI drive reliable and heritable individual differences in functional brain networks. Neuroimage 189, 516–532.

Fair, D.A., Schlaggar, B.L., Cohen, A.L., Miezin, F.M., Dosenbach, N.U.F., Wenger, K.K., Fox, M.D., Snyder, A.Z., Raichle, M.E., Petersen, S.E., 2007. A method for using blocked and

event-related fMRI data to study "resting state" functional connectivity. Neuroimage 35, 396–405.

Fornito, A., Bullmore, E.T., 2015. Connectomics: a new paradigm for understanding brain disease. Eur. Neuropsychopharmacol. 25, 733–748.

Glasser, M.F., Coalson, T.S., Robinson, E.C., Hacker, C.D., Harwell, J., Yacoub, E., Ugurbil, K., Andersson, J., Beckmann, C.F., Jenkinson, M., Smith, S.M., Van Essen, D.C., 2016. A multi-modal parcellation of human cerebral cortex. Nature 536, 171–178.

Glasser, M.F., Sotiropoulos, S.N., Wilson, J.A., Coalson, T.S., Fischl, B., Andersson, J.L., Xu, J., Jbabdi, S., Webster, M., Polimeni, J.R., Van Essen, D.C., Jenkinson, M., WU-Minn HCP Consortium, 2013. The minimal preprocessing pipelines for the Human Connectome Project. Neuroimage 80, 105–124.

Gordon, E.M., Laumann, T.O., Adeyemo, B., Petersen, S.E., 2015. Individual Variability of the System-Level Organization of the Human Brain. Cereb. Cortex bhv239.

Gordon, E.M., Laumann, T.O., Gilmore, A.W., Newbold, D.J., Greene, D.J., Berg, J.J., Ortega, M., Hoyt-Drazen, C., Gratton, C., Sun, H., Hampton, J.M., Coalson, R.S., Nguyen, A.L., McDermott, K.B., Shimony, J.S., Snyder, A.Z., Schlaggar, B.L., Petersen, S.E., Nelson, S.M., Dosenbach, N.U.F., 2017. Precision Functional Mapping of Individual Human Brains. Neuron 95, 791–807.e7.

Gratton, C., Laumann, T.O., Nielsen, A.N., Greene, D.J., Gordon, E.M., Gilmore, A.W., Nelson, S.M., Coalson, R.S., Snyder, A.Z., Schlaggar, B.L., Dosenbach, N.U.F., Petersen, S.E., 2018. Functional Brain Networks Are Dominated by Stable Group and Individual Factors, Not Cognitive or Daily Variation. Neuron 98, 439–452.e5.

Hutchison, R.M., Womelsdorf, T., Allen, E.A., Bandettini, P.A., Calhoun, V.D., Corbetta, M., Della Penna, S., Duyn, J.H., Glover, G.H., Gonzalez-Castillo, J., Handwerker, D.A., Keilholz, S., Kiviniemi, V., Leopold, D.A., de Pasquale, F., Sporns, O., Walter, M., Chang, C., 2013. Dynamic functional connectivity: promise, issues, and interpretations. Neuroimage 80, 360–378.

Krause, F., Benjamins, C., Eck, J., Lührs, M., van Hoof, R., Goebel, R., 2019. Active head motion reduction in magnetic resonance imaging using tactile feedback. Hum. Brain Mapp. 40, 4026–4037.

Kumar, A., Lin, F., Rajapakse, J.C., 2016. Mixed Spectrum Analysis on fMRI Time-Series. IEEE Trans. Med. Imaging 35, 1555–1564.

Laumann, T.O., Gordon, E.M., Adeyemo, B., Snyder, A.Z., Joo, S.J., Chen, M.-Y., Gilmore, A.W., McDermott, K.B., Nelson, S.M., Dosenbach, N.U.F., Schlaggar, B.L., Mumford, J.A., Poldrack, R.A., Petersen, S.E., 2015. Functional System and Areal Organization of a Highly Sampled Individual Human Brain. Neuron 87, 657–670.

Marcus, D.S., Harms, M.P., Snyder, A.Z., Jenkinson, M., Wilson, J.A., Glasser, M.F., Barch, D.M., Archie, K.A., Burgess, G.C., Ramaratnam, M., Hodge, M., Horton, W., Herrick, R., Olsen, T., McKay, M., House, M., Hileman, M., Reid, E., Harwell, J., Coalson, T., Schindler, J., Elam, J.S., Curtiss, S.W., Van Essen, D.C., WU-Minn HCP Consortium, 2013. Human Connectome Project informatics: quality control, database services, and data visualization. Neuroimage 80, 202–219.

Matheson, G.J., 2019. We need to talk about reliability: making better use of test-retest studies for study design and interpretation. PeerJ. https://doi.org/10.7717/peerj.6918

Meissner, T.W., Walbrin, J., Nordt, M., Koldewyn, K., Weigelt, S., 2020. Head motion during fMRI tasks is reduced in children and adults if participants take breaks. bioRxiv.

https://doi.org/10.1101/816116

Menon, V., Lim, K.O., Anderson, J.H., Johnson, J., Pfefferbaum, A., 1997. Design and efficacy of a head-coil bite bar for reducing movement-related artifacts during functional MRI scanning. Behav. Res. Methods Instrum. Comput. 29, 589–594.

Noble, S., Scheinost, D., Constable, R.T., 2019. A decade of test-retest reliability of functional connectivity: A systematic review and meta-analysis. Neuroimage 203, 116157.

Noble, S., Spann, M.N., Tokoglu, F., Shen, X., Constable, R.T., Scheinost, D., 2017. Influences on the Test–Retest Reliability of Functional Connectivity MRI and its Relationship with Behavioral Utility. Cereb. Cortex 27, 5415–5429.

O'Connor, D., Potler, N.V., Kovacs, M., Xu, T., Ai, L., Pellman, J., Vanderwal, T., Parra, L.C., Cohen, S., Ghosh, S., Escalera, J., Grant-Villegas, N., Osman, Y., Bui, A., Cameron Craddock, R., Milham, M.P., 2017. The Healthy Brain Network Serial Scanning Initiative: a resource for evaluating inter-individual differences and their reliabilities across scan conditions and sessions. GigaScience. https://doi.org/10.1093/gigascience/giw011

Parkes, L., Fulcher, B., Yücel, M., Fornito, A., 2018. An evaluation of the efficacy, reliability, and sensitivity of motion correction strategies for resting-state functional MRI. Neuroimage 171, 415–436.

Power, J.D., Plitt, M., Laumann, T.O., Martin, A., 2017. Sources and implications of whole-brain fMRI signals in humans. Neuroimage 146, 609–625.

Schmälzle, R., Imhof, M.A., Grall, C., Flaisch, T., Schupp, H.T., 2017. Reliability of fMRI time series: Similarity of neural processing during movie viewing. bioRxiv.

Shah, L.M., Cramer, J.A., Ferguson, M.A., Birn, R.M., Anderson, J.S., 2016. Reliability and reproducibility of individual differences in functional connectivity acquired during task and resting state. Brain Behav. 6, e00456.

Smith, S.M., Vidaurre, D., Beckmann, C.F., Glasser, M.F., Jenkinson, M., Miller, K.L., Nichols, T.E., Robinson, E.C., Salimi-Khorshidi, G., Woolrich, M.W., Barch, D.M., Uğurbil, K., Van Essen, D.C., 2013. Functional connectomics from resting-state fMRI. Trends Cogn. Sci. 17, 666–682.

Van Essen, D.C., Smith, S.M., Barch, D.M., Behrens, T.E.J., Yacoub, E., Ugurbil, K., WU-Minn HCP Consortium, 2013. The WU-Minn Human Connectome Project: an overview. Neuroimage 80, 62–79.

Xu, T., Opitz, A., Craddock, R.C., Wright, M.J., Zuo, X.-N., Milham, M.P., 2016. Assessing Variations in Areal Organization for the Intrinsic Brain: From Fingerprints to Reliability. Cereb. Cortex. https://doi.org/10.1093/cercor/bhw241

Xu, T., Yang, Z., Jiang, L., Xing, X.-X., Zuo, X.-N., 2015. A Connectome Computation System for discovery science of brain. Sci Bull. Fac. Agric. Kyushu Univ. 60, 86–95.

Yeo, B.T.T., Krienen, F.M., Sepulcre, J., Sabuncu, M.R., Lashkari, D., Hollinshead, M., Roffman, J.L., Smoller, J.W., Zöllei, L., Polimeni, J.R., Fischl, B., Liu, H., Buckner, R.L., 2011. The organization of the human cerebral cortex estimated by intrinsic functional connectivity. J. Neurophysiol. 106, 1125–1165.

Zou, G.Y., 2012. Sample size formulas for estimating intraclass correlation coefficients with precision and assurance. Statistics in Medicine. https://doi.org/10.1002/sim.5466

Zuo, X.N., Anderson, J.S., Bellec, P., Birn, R.M., Biswal, B.B., Blautzik, J., Breitner, J.C., Buckner, R.L., Calhoun, V.D., Castellanos, F.X., Others, 2014. An open science resource for establishing reliability and reproducibility in functional connectomics. Sci. Data 1, 140049.

Zuo, X.-N., Anderson, J.S., Bellec, P., Birn, R.M., Biswal, B.B., Blautzik, J., Breitner, J.C.S.,
    Buckner, R.L., Calhoun, V.D., Castellanos, F.X., Chen, A., Chen, B., Chen, J., Chen, X.,
    Colcombe, S.J., Courtney, W., Craddock, R.C., Di Martino, A., Dong, H.-M., Fu, X., Gong,
    Q., Gorgolewski, K.J., Han, Y., He, Y., He, Y., Ho, E., Holmes, A., Hou, X.-H., Huckins,
    J., Jiang, T., Jiang, Y., Kelley, W., Kelly, C., King, M., LaConte, S.M., Lainhart, J.E., Lei,
    X., Li, H.-J., Li, K., Li, K., Lin, Q., Liu, D., Liu, J., Liu, X., Liu, Y., Lu, G., Lu, J., Luna,
    B., Luo, J., Lurie, D., Mao, Y., Margulies, D.S., Mayer, A.R., Meindl, T., Meyerand, M.E.,
    Nan, W., Nielsen, J.A., O'Connor, D., Paulsen, D., Prabhakaran, V., Qi, Z., Qiu, J., Shao,
    C., Shehzad, Z., Tang, W., Villringer, A., Wang, H., Wang, K., Wei, D., Wei, G.-X., Weng,
    X.-C., Wu, X., Xu, T., Yang, N., Yang, Z., Zang, Y.-F., Zhang, L., Zhang, Q., Zhang, Z.,
    Zhang, Z., Zhao, K., Zhen, Z., Zhou, Y., Zhu, X.-T., Milham, M.P., 2014. An open science
    resource for establishing reliability and reproducibility in functional connectomics. Sci Data
    1, 140049.
Zuo, X.-N., Xu, T., Milham, M.P., 2019. Harnessing reliability for neuroscience research. Nat
    Hum Behav 3, 768–771.