

1 Conscious processing of narrative 2 stimuli synchronizes heart rate 3 between individuals

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41 Abstract

42 Heart rate has natural fluctuations that are typically ascribed to autonomic function. Recent
43 evidence suggests that conscious processing can affect the timing of the heartbeat. We
44 hypothesized that heart rate is modulated by conscious processing and therefore dependent
45 on attentional focus. To test this we leverage the observation that neural processes can be
46 synchronized between subjects by presenting an identical narrative stimulus. As predicted, we
47 find significant inter-subject correlation of the heartbeat (ISC-HR) when subjects are presented
48 with an auditory or audiovisual narrative. Consistent with the conscious processing hypothesis,
49 we find that ISC-HR is reduced when subjects are distracted from the narrative, and that higher
50 heart rate synchronization predicts better recall of the narrative. Finally, patients with disorders
51 of consciousness who are listening to a story have lower ISC, as compared to healthy
52 individuals, and that individual ISC-HR might predict a patients' prognosis. We conclude that
53 heart rate fluctuations are partially driven by conscious processing, depend on attentional
54 state, and may represent a simple metric to assess conscious state in unresponsive patients.

55 Introduction

56 In healthy individuals, heart rate fluctuates with breathing and changes in parasympathetic and
57 sympathetic tone¹⁻³. Physical activity naturally increases heart rate, but also just thinking about
58 physical activity may increase heart rate⁴. Similarly, mental exercises such as meditation can
59 reduce heart rate⁵. The effect of cognition on heart rate is perhaps even more direct than these
60 traditional accounts^{6,7}. We also know that suspense and surprise can transiently increase heart
61 rate⁸. Most likely these immediate effects of the mind on the heart subserved the purpose of
62 preparing the body for imminent action⁹. Despite this evidence, the role of conscious
63 perception¹⁰ on heart rate is less clear. It is well established that the brain can unconsciously
64 detect novelty in the stimulus, as demonstrated with event-related potential studies (e.g.
65 MMN¹¹⁻¹³, and N400^{14,15}). Recent evidence shows that the timing of an individual heartbeat
66 may be affected by the perception of an unexpected sound, but only when consciously
67 perceived¹⁶. We hypothesize that conscious processing of perceptual information will affect
68 heart rate. Therefore, we predict that fluctuations in heart rate will depend on top-down
69 attention to the stimulus and predict memory performance, a known factor¹⁷ and a correlate of
70 conscious perception.¹⁸

71 To test these predictions we will leverage the observation that natural narrative stimuli guide
72 cognitive processes resulting in reliable neural responses. This was first observed by
73 measuring hemodynamic brain activity during movies: when humans watch the same movie,
74 they have similar fluctuations in brain blood oxygenation¹⁹. Specifically, the temporal
75 fluctuations of the signal measured with functional magnetic resonance (fMRI) are correlated
76 between subjects. Significant inter-subject correlation of brain activity has now been observed
77 with other neuroimaging modalities, including EEG, MEG and fNIRS¹⁰⁻¹³. Thus,
78 neurophysiological fluctuations appear to synchronize on a wide range of time scales, from
79 milliseconds to several minutes. This phenomenon is also not constrained to movies but has
80 been observed for speech, music, or during driving²⁰⁻²². There are even significant correlations
81 in the spatial patterns of fMRI activity between speakers and listeners²³ or the time-courses of
82 EEG signals of two individuals engaged in a conversation²⁴. This similarity of neural activity in

83 response to narrative stimuli suggests that these stimuli elicit similar perceptual and cognitive
84 processes in different subjects.

85 Consistent with this, inter-subject correlation crucially depends on the cognitive state of the
86 participant. Subjects that are not attentive or do not follow the narrative show significantly
87 reduced inter-subject correlation, both in EEG and fMRI²⁵⁻²⁷. A drop in inter-subject correlation
88 is also observed in patients with disorders of consciousness relative to healthy controls²⁸⁻³⁰.
89 Indeed, a cohesive narrative is crucially important to elicit synchronized brain activity in fMRI,
90 in particular at long time scales.³¹ It comes as no surprise then that inter-subject correlation
91 has been found to be predictive of a variety of behavioral outcomes, such as audience
92 retention, memory of content, efficacy of advertising, efficacy of communication and political
93 speeches, and more^{23,25,32-35}.

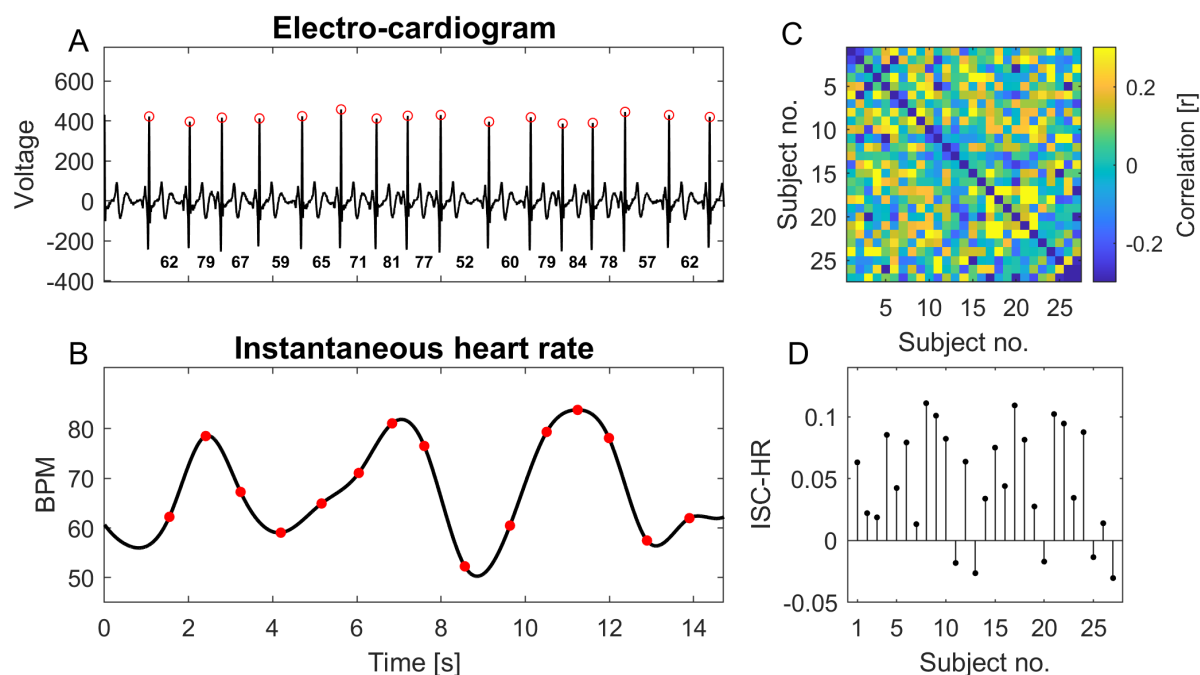
94 There are many studies reporting a correlation of physiological signals across subjects.³⁶
95 Generally this has been linked to physical or social interaction,³⁷⁻⁴⁰ or at the very least a co-
96 presence at the same place and time.⁴¹ However, consistent with our hypothesis, the
97 simultaneous experience is not crucial for synchronization. A few recent studies report a
98 correlation of heart rate fluctuations across subjects watching the same movie at different
99 times, and ascribe this to shared emotions elicited by the film.^{42,43}

100 Our conscious processing hypothesis predicts that this synchronization phenomenon will occur
101 not just for the film, but more generally for narrative stimuli, that inter-subject correlation of
102 heart rate will be modulated by attention, that it will correlate with cognitive performance, and
103 more dramatically, that it will be reduced in patients with disorders of consciousness. We
104 confirm these predictions in a series of four experiments and conclude that heart rate
105 synchronization has the potential to become a marker of cognitive state in a clinical setting.

106 Results

107 In all four experiments we presented narrative stimuli to each subject while recording their
108 electrocardiogram (EKG, Figure 1A). Recordings were aligned in time between subjects and
109 instantaneous HR was estimated as the inverse of the RR intervals (Figure 1B). Mean and
110 standard deviation of these instantaneous measures provide HR and HR variability (HRV) for
111 each subject. The instantaneous HR signals are upsampled to a common sampling rate and
112 correlated between all pairs of subjects (Figure 1C). Inter-subject correlation of HR (ISC-HR)
113 is then defined for each subject as the average Pearson's correlation with all other subjects
114 (Figure 1D).

115



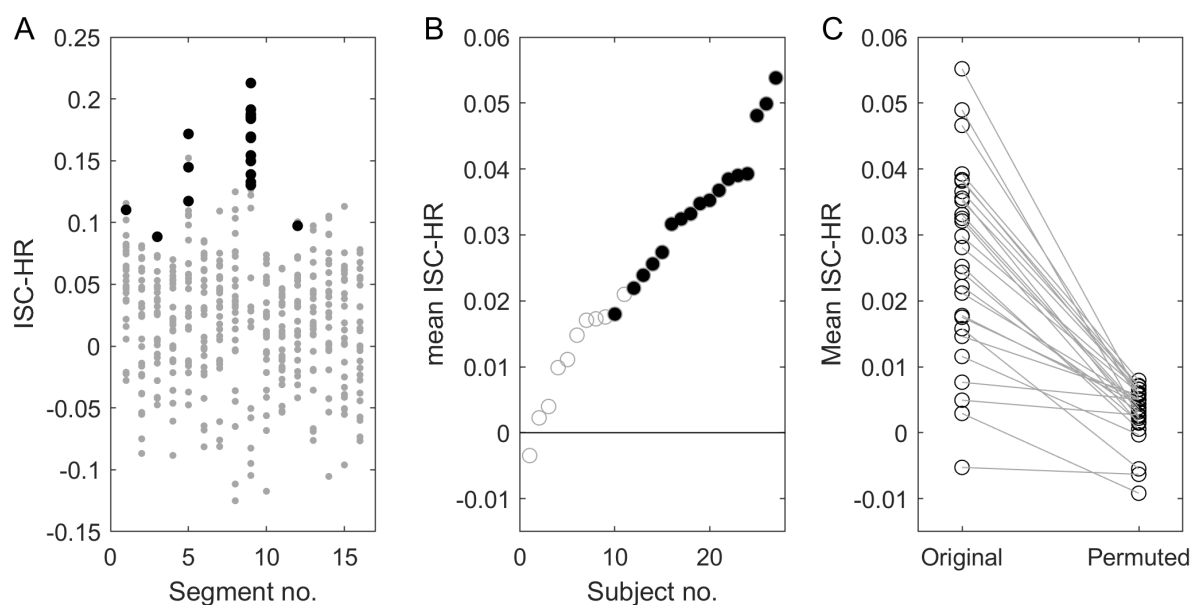
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117 **Figure 1: Inter subject correlation of heart rate (ISC-HR),** **A:** Electro-cardiogram with peak of the R-
118 wave detected (red o). **B:** The inverse of the interval between two R-waves defines the instantaneous
119 heart rate (red o). This is interpolated (black) to convert heart rate into a signal with a uniform sampling
120 rate across subjects. **C:** Pearson's correlation coefficient of this instantaneous heart rate between
121 pairs of subjects. **D:** Inter-subject correlation of heart rate (ISC-HR) is computed for each individual as
122 the mean across a row of this correlation matrix. Example in this figure is taken from history segment
123 #1, dataset #1.

124 Auditory narratives synchronize listeners' heart rate fluctuations

125 The objective of the first experiment was to determine whether a common auditory narrative
126 elicits similar heart rate fluctuations in healthy volunteers (Experiment 1). Subjects were
127 presented with one-minute segments of an audiobook of Jules Verne's "20,000 leagues under
128 the sea". First we tested whether there was significant inter-subject correlation of the
129 instantaneous HR. To this end we compared the ISC-HR values to values computed on signals
130 randomly shifted in time within-subjects (see methods). When this analysis is performed on
131 individual one-minute segments, only a few subjects show significant non-zero ISC-HR (Fig.
132 2A, red dots, FDR at 0.05). When averaging ISC-HR values over the 16 minutes, 17 of the 27
133 subjects show statistically significant HR correlation (Fig. 2B; FDR at 0.05). No significant
134 negative correlations were found. As an additional control, we randomly shuffle the one-minute
135 story segments between subjects breaking the narrative synchrony across subjects. As
136 expected, we observed a drop in ISC with values no longer statistically significant (Fig. 2C). In
137 total, we conclude that the narrative stimulus induces similar HR fluctuations across subjects.
138 ISC-HR therefore captures how strongly the stimulus drives the fluctuations of HR in each
139 subject.

140 Results on average HR and HRV and their potential relation to ISC-HR are generally
141 unremarkable for these data and are discussed in the Supplement (Fig. S1).



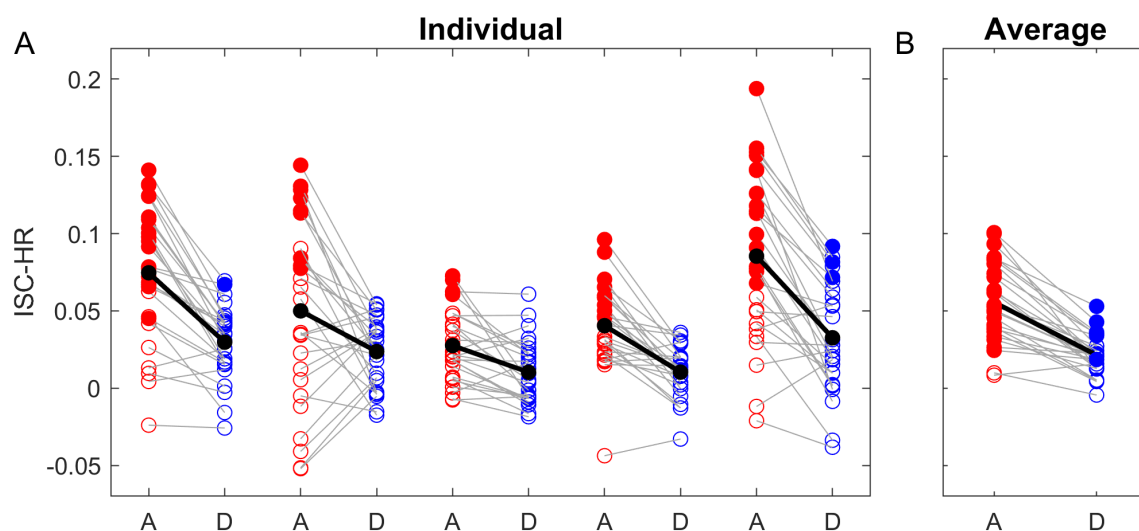
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143 **Figure 2: ISC-HR resolved in time and by subject.** In Experiment 1, subjects listened to segments of
144 audio narratives of 60 seconds each (N=16). **A:** ISC-HR is computed for each subject (N=27) and each
145 segment. **B:** For each of the 27 subjects ISC is averaged over the 16 segments. Subjects are ordered
146 by their ISC values. Black points (panel A and B) indicate statistically significant ISC values. Gray points
147 are not statistically significant. Statistical significance is determined using circular shuffle statistics
148 (10,000 shuffles and corrected for multiple comparisons with FDR of 0.01). Specifically, the heart rate
149 signal of each subject is randomly shifted in time. **C:** As additional control here ISC is compared to the
150 ISC obtained when story segments are swapped across subjects at random.

151 **Attention modulates synchronization of HR fluctuations during audiovisual narratives**

152 We demonstrated above that an auditory narrative can synchronize HR fluctuations across
153 subjects. In the second experiment we aim to determine if this synchronization is modulated
154 by attention to the stimulus (Experiment 2). Here we used short and engaging instructional
155 videos of 3-5 minute duration, similar to our previous work²⁷. Each subject viewed 5 videos in
156 sequence normally. Then they view the same videos a second time, but now with the instruction
157 to count backward silently in their mind in step 7 starting from a random number. This
158 secondary task aims to distract subjects from viewing the video^{26,27}.

159 We find that ISC-HR drops in the distracted condition relative to the normal attentive state (Fig.
160 3A). A repeated-measures ANOVA shows a strong effect of attention ($F(1,238)=73.45$,
161 $p=1.32e-15$) and an effect of the video ($F(4,238)=14.59$, $p=1.14e-10$) as well as a subject effect
162 ($F(26,238)=2.86$, $p=1.34e-05$). The effect of attention is significant for each story individually
163 (follow up pairwise t-test, all $p<0.05$) and when averaging over all 5 videos with a total duration
164 of 22:33 minutes we see a numerical drop in ISC-HR with distraction in all but one of the 27
165 subjects (Fig. 3B).



166

167 **Figure 3: Intersubject correlation (ISC) of the instantaneous heart rate is modulated by attention.**

168 In Experiment 2, 27 subjects watched 5 educational videos of 3-5 minute duration each. Here ISC is
169 measured against the attentive condition, i.e. both attentive and distracted subjects are correlated
170 against the HR collected during the attentive condition. Filled points indicate individually statistically
171 significant ISC-HR (FDR < 0.01). **A:** Subjects watched the same videos twice, either in an attentive (A,
172 red) or distracted (D, blue) condition. ISC was systematically higher in the attentive condition for the five
173 videos. Gray lines indicate individual subjects and the black lines the group average. **B:** Same results
174 when average across the five videos.

175

176 **Attention modulates HRV, but this is not the driving factor in modulation of ISC**

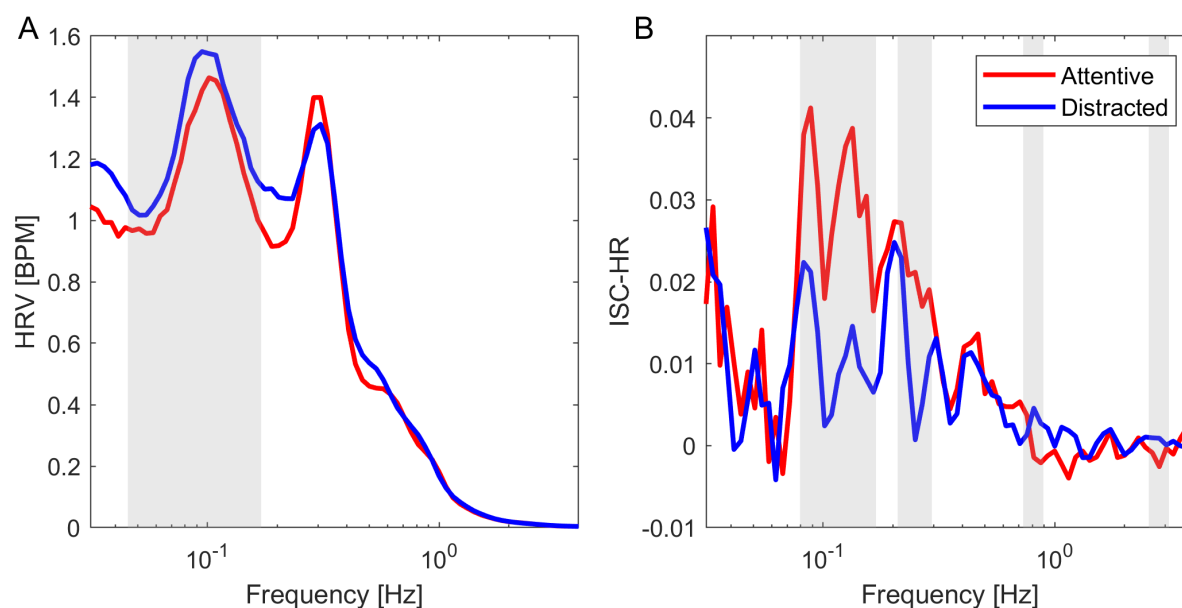
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178 For this Experiment 2, in addition to ISC we also analyzed heart rate variability (HRV), defined
179 here as the standard deviation of instantaneous HR (Fig. S2B). We see an increase in HRV
180 when subjects are distracted. An ANOVA shows a fixed effect of attention ($F(1,211)=63.60$,
181 $p=9.54e-14$), random effect of subject ($F(23,211)=29.56$, $p=1.57e-53$), but we see no
182 significant video effect ($F(4,211)=0.77$, $p=5.44e-01$). Perhaps the increase in HRV in the
183 distracted condition could explain the drop in ISC-HR. If this was the case, we would expect
184 that HRV correlates negatively with ISC-HR as, by definition, the two are inversely related.
185 However, the opposite seems to be the case: subjects with higher HRV have also higher ISC-
186 HR (Fig. S2D). Therefore, it appears that the modulation of HRV and ISC-HR are independent
187 phenomena. The effects on mean HR were generally unremarkable (Fig. S2A & S2C).

188

189 **Synchronization of HR fluctuations is modulated in the time scale of 5-10 seconds**

190 It is well established that HR fluctuates at different timescales⁴⁴. This is confirmed on the
191 present data (of Experiment 2) by computing HRV after band-pass filtering the instantaneous
192 HR in different frequency bands (Fig. 4A). To determine which time scale dominates ISC and
193 its modulation with attention we computed ISC similarly resolved by frequency band (Fig. 4B).
194 We find that ISC and its modulation with attention are dominant in the mid-frequency range --
195 from 0.1 Hz to 0.2 Hz in this study -- a range of HR fluctuations that are known to disappear
196 during slow-wave sleep⁴⁵.



197
198 **Figure 4. Spectrum of instantaneous HR and ISC-HR and its modulation with attention.** For
199 Experiment 2, instantaneous HR was band-pass filtered with center frequency on a logarithmic scale
200 and a bandwidth of 0.2 of the center frequency. **A:** HRV is computed here as the root mean square of
201 the band-passed instantaneous HR averaged over the 5 videos (~15 min total). **B:** ISC-HR is computed
202 as before, but now on the band-passed instantaneous HR and averaged over the 5 videos. In both
203 panels significant differences between attending and distracted conditions are established in each band
204 with a paired t-test over the 27 subjects (grey shaded area indicates $p < 0.05$, uncorrected).
205

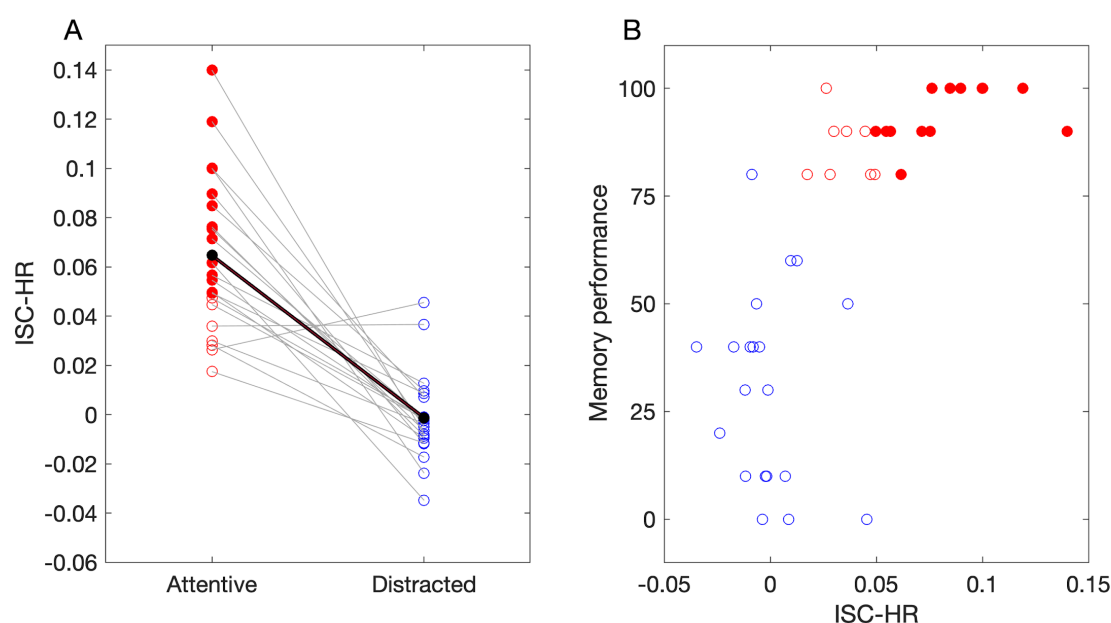
206 **Attention modulates synchronization of HR fluctuations during audio-only narratives,** 207 **but does not synchronize breathing**

208 Given the dependence of HR fluctuations on attention, we expected that HR would be
209 predictive of cognitive processing of the narrative. In the next experiment (Experiment 3) we,
210 therefore, recorded HR during the presentation of auditory narratives, and afterward asked
211 adult subjects to recall factual information presented in the story, e.g. “What was the name of
212 the two main characters?”. Subjects listened to four auditory narratives, in either an attentive
213 or distracted condition. This time the narratives were children’s stories of 8-11 minute duration,
214 and the secondary task consisted of counting target tones that were inserted in the audio
215 asynchronously across subjects. To rule out order effects we now divided the participants in
216 two groups. In group 1 (N=9) subjects listened to stories 1 and 2 in the attentive condition and
217 stories 3 and 4 in the distracted condition. In group 2 (n=12) subject listened to the same stories
218 with the attention condition reversed.

219 We find again that ISC-HR drops significantly when subjects are distracted (Fig. 5A, paired t-
220 test $t(21)=8.2$, $p < 10^{-7}$). Similarly to experiment 2 with video, here 15 out of the 21 subjects
221 show a statistically significant correlation of HR in the attentive condition and none in the
222 distracted condition. As expected, subjects performed significantly better in recalling elements
223 of the story in the attentive condition as compared to the distracted condition (Supplementary
224 Fig. S3, Wilcoxon Signed-Rank Test, $z = 4.03$, $p = 5.7e-5$).

225 Our hypothesis postulates that ISC-HR is the result of similar conscious processing of the
226 narrative stimulus, thus, we predicted that subjects with higher ISC-HR will be better at

227 remembering elements of the stories. Indeed, we find that ISC correlates with memory recall
228 performance across conditions (Fig 5B, $r(40)=0.767$, $p=3.1e-9$, Spearman's correlation is used
229 here due to the bounded nature of the percent measure). More importantly, even within the
230 normally attentive condition with a normal fluctuation of HR we find that ISC-HR is predictive
231 of memory performance ($r(19)=0.57$, $p=7.3 e-3$). In the distracted conditions there was no
232 correlation with memory performance ($r(19)=-0.1$, $p=0.67$) possibly because ISC-HR was not
233 statistically significant for any of the subjects. Overall we conclude that ISC-HR is indicative of
234 conscious processing of the narrative.



235

236 **Figure 5: Intersubject correlation is higher when subjects were attentive to the auditory narrative**
237 **and this correlation indexes the subjects' memory performance.** In Experiment 3, Subjects listened
238 to four recordings of children's stories 8-10 minutes in duration. Subjects were instructed to either attend
239 to a story normally (attentive, red), or to count backward when they heard a target sound inserted in the
240 audio (distracted, blue). Again ISC is measured against the attentive condition, i.e. both attentive and
241 distracted subjects are correlated against the HR collected during the attentive condition. Filled points
242 indicate individually statistically significant ISC-HR (FDR < 0.01). **A:** ISC-HR for each subject (N=21)
243 averaged over four stories. **B:** Memory performance measured as percent of correct answers to free
244 recall questions about the content of the stories. Filled and empty circles indicate significant and non-
245 significant ISC-HR respectively ($p < 0.05$ shuffle statistics)
246

247 Intersubject correlation of heart rate is not driven by synchronous breathing

248 It is well established that HR fluctuations are driven in part by breathing. This phenomenon is
249 known as respiratory sinus arrhythmia and is strongest in the frequency band around 0.1 Hz.⁴⁶
250 It is possible that the attentional modulation in this frequency band is caused by
251 synchronization of breathing between subjects. We, therefore, collected in Experiment 3 also
252 respiratory movement concurrently with the EKG and measured inter-subject correlation of
253 breathing (Supplementary Fig. S5A). We did not find a significant ISC of breathing in any of
254 the subjects, nor was there any effect of attention when comparing across all subjects (paired
255 t-test, $t(21)=0.5$, $p=0.6$). In other words, the auditory narratives did not reliably entrain the
256 subjects breathing nor was this modulated by attention. Interestingly, breathing does

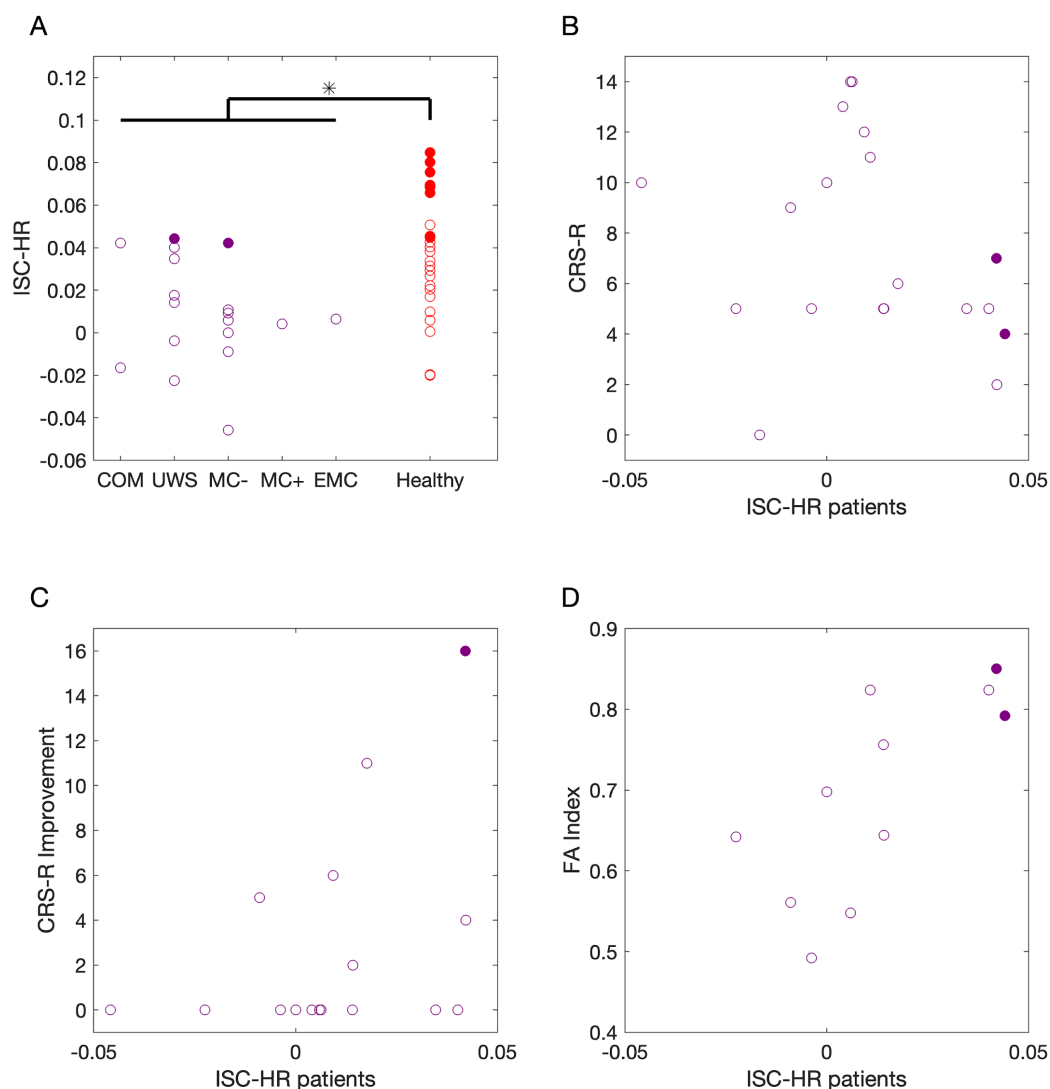
257 significantly correlate with HR (Supplementary Figure S5B, $t(20)=4.49$, $p=2e-4$) reflecting the
258 well-established respiratory sinus arrhythmia. In addition, we found a reduction breathing-HR
259 correlation in the distracted condition versus the attentive condition but it didn't reach statistical
260 significance ($t(20)=1.86$, $p=0.08$), suggesting that this link does not depend on attention. In
261 conclusion, these results suggest that the effect of cognition on instantaneous HR is not related
262 to breathing.

263 **Synchronization of heart rate fluctuations is disrupted in patients with disorder of** 264 **consciousness**

265 Given the dependence on attention and conscious processing of these synchronized HR
266 fluctuations, we predicted that patients with disorders of consciousness (DOC) will have
267 diminished HR synchronization when presented with an auditory narrative. We recorded EKG
268 in 19 DOC patients, in addition to 24 healthy controls (Experiment 4). The patients were
269 hospitalized to determine their state of consciousness and neurological prognosis. Patients
270 were behaviorally assessed using the standard Coma Recovery Scale-revised⁴⁷. State of
271 consciousness was determined using the currently accepted categorization⁴⁸, patients were
272 classified either in (1) Coma, (2) Vegetative state/Unresponsive wakefulness syndrome
273 (UWS), (3) Minimally conscious state minus (MCS-), (4) Minimally conscious state plus
274 (MCS+), and exit Minimally conscious state (EMCS). Patients and healthy subjects listened
275 through headphones to a children's story of 10-minute duration. ISC-HR was calculated by
276 correlating HR with that of healthy controls. As expected ISC-HR values were lower in patients
277 (t -test: $t(41) = 3.14$, $p = 0.003$, Fig. 6A). Within patients no significant correlation was found
278 between ISC-HR and state-of-consciousness (Fig. 6A, Spearman correlation, $R(17) = -0.28$, p
279 $= 0.24$) nor between ISC-HR and the Coma Recovery Scale-Revised (CRS-R⁴⁷; Fig 6B,
280 Spearman correlation, $R(17) = -0.3$, $p = 0.22$). Reduced HRV is sometimes found in traumatic
281 brain injury patients.⁴⁹ We therefore analyzed HRV to verify that the drop in ISC-HR is not a
282 noise-floor effect, i.e. if HRV drops in patients it may be difficult to measure inter-subject
283 correlation above random fluctuations (Fig. S6B). Contrary to what was expected we found
284 higher HRV in the DOC patients compared to healthy controls ($t(41) = 2.34$, $p = 0.02$), ruling
285 out a noise-floor effect. We also found higher mean HR in DOC patients compared to healthy
286 controls (Fig S6A; $t(41) = 4.7$, $p = 2.9e-05$). However, given the previous lack of correlation
287 between ISC and mean HR we do not believe this contributed to the decrease of ISC-HR in
288 patients.

289 When measured individually, only two of 19 patients showed statistically significant ISC-HR
290 (FDR corrected $p < 0.05$, Fig. 6, purple filled circles). For these two patients outcomes at the
291 six-month follow-up were mixed; one patient fully regained consciousness whereas for the
292 other, life-sustaining therapies were withdrawn before the follow-up assessment. Among the
293 remaining 17 patients only one additional patient recovered consciousness, although in a
294 completely aphasic condition. These results suggest that the patients' ISC-HR might carry
295 prognostic information with a specific emphasis on conscious verbal processing. To test this
296 hypothesis we first correlated the patients' ISC-HR to the CRS-R improvement after six months
297 of the initial assessment. We found a positive correlation between ISC-HR and CRS-R
298 improvement, although not statistically significant (Fig 6C, Spearman correlation,
299 $R(14)=0.43$, $p=0.097$, second assessment was available only for 16 patients). A limitation of
300 behavioral assessment of patients is that it cannot detect covert awareness^{50,51}, a condition
301 that can occur in up to 15% of the UWS patients⁵². Therefore, we also correlated the patients'

302 ISC-HR to an anatomical measure of brain integrity -- whole-brain white matter fractional
303 anisotropy. This FA index has been linked to neurological recovery in DOC patients⁵³. We
304 found a significant correlation between ISC-HR and FA Index (Fig. 6D, Spearman correlation,
305 $R(9)=0.73, p=0.01$, FA Index was available only for 11 patients).



306

307 **Figure 6: Audio narratives synchronize HR fluctuations in healthy controls but not in**
308 **patients with disorder of consciousness.** In Experiment 4, subjects listened to a children's
309 story (La part des ancêtres from Leonora Miano; 10 minutes). **A:** ISC-HR is measured by
310 correlating instantaneous HR with that of healthy subjects. Filled cycles indicated statistically
311 significant ISC. **B:** Comparison of the ISC-HR with Coma Recovery Scale-Revised in patients
312 (N=19). **C:** Comparison of the ISC-HR with improvement of Coma Recovery Scale-Revised six
313 months after the first assessment (N=17) **D:** Comparison of ISC-HR and whole-brain white
314 matter fractional anisotropy in patients, were available (N=11).

315 Discussion

316 The hypothesis that motivated this set of experiments was that conscious processing of
317 information modulates instantaneous heart rate. This fluctuating heart rate will synchronize

318 across subjects when presented with narrative stimuli that are processed similarly. We tested
319 the predictions resulting from this hypothesis in a series of four experiments. In the first
320 experiment with healthy volunteers we confirmed that heart rate fluctuations correlate between
321 subjects for auditory narratives. In the second and third experiment we confirm that distracting
322 the participants with a secondary task reduced this correlation, for video and audio narratives
323 alike. Importantly, we confirm the prediction that synchronization of HR fluctuations is predictive
324 of memory performance. We also determined that HR synchronization is not driven by
325 synchronous breathing across subjects. Finally, in the fourth experiment we presented an
326 auditory narrative to patients with disorders of consciousness and found that their heart rate
327 fluctuations do not correlate with that of healthy subjects.

328
329 There is an extensive literature demonstrating that physiological signals such as heart rate,
330 respiration, and skin conductivity can synchronize between individuals.³⁶ This literature
331 emphasizes physical interaction and social relationships as the factors driving this
332 synchronization. Even in the context of music, theater, or film, the emphasis is on the
333 concurrent and shared experience of an audience that synchronizes heart rate to one-
334 another.^{37–39,54} Here we have emphasized instead that it is the stimulus that synchronizes HR,
335 or more precisely, a similar processing of a common stimulus. There is no need for individuals
336 to directly interact, be related to one another or perceive the stimulus together at the same
337 time. Consistent with our hypothesis, previous reports already show that emotional movies
338 can synchronize the HR of viewers, even when watching the movie individually.^{42,43} The
339 present findings go beyond this previous literature in that this HR synchronization
340 phenomenon is not specific to live experiences or emotional movies. Rather, it occurs with
341 many narrative stimuli, as we demonstrated here with audio recordings of children’s stories or
342 animated educational videos.

343
344 There is also an extensive literature on the inter-subject correlation of brain signals evoked by
345 dynamic natural stimuli, starting with experiments in fMRI while subjects watched movies.¹⁹
346 This work demonstrated that subjects process natural stimuli similarly, and that similarity of
347 brain activity is predictive of memory performance.⁵⁵ Subsequent experiments replicated these
348 findings with EEG.^{56,57} Additionally, ISC of EEG is reduced when subjects are distracted²⁶ and
349 is reduced in patients with disorder of consciousness,⁵⁸ similar to what we find here with the
350 instantaneous heart rate. Given these parallels we expect that HR fluctuations will also
351 synchronize across subjects listening to engaging music,²¹ and that HR synchronization will
352 be a good indication of how engaging a narrative is.^{32,59}

353
354 We suggest that some previous work on physiological synchronization of autonomic signals
355 can be reinterpreted in the context of the present conscious processing hypothesis. For
356 example, the same performance is judged differently depending on the social relationship of
357 performer and audience member, suggesting that it is a different way of processing information
358 in the audience member.³⁷ In our view, it is the processing of the common stimulus, and not
359 the co-presence in the same physical space that causes the synchronization of the heart rate
360 fluctuations. We predict that many results obtained with live performances^{37–39} or in-person
361 interactions²⁶ could be recovered with asynchronous playback of the same experience
362 recorded with video. Evidently the experience may be less powerful than live in-person
363 experiences,⁴¹ but the modulating factors of relationships, emotions, or empathy may still
364 prevail in this virtual context.

365

366 We postulate that factors intrinsic to the story, such as semantics and emotions, driving a
367 synchronized heart rate. This may include semantics of single-word to syntactic and multi-
368 sentence level of representation as well as prosody, valence of single words, and more
369 complex semantically mediated emotions. Capturing semantics and emotions require
370 attention to the stimulus and some level of language comprehension. In this view, it is the
371 narrative content that drives attention, engagement, interest and emotions. It is possible,
372 indeed likely that the variations in ISC are due to this differing narrative content. Indeed we
373 find a strong difference in ISC between stimuli, even within the same type of animated
374 educational videos. Dependence of ISC on the stimulus has been found in previous EEG
375 studies^{32,35,60} and for heart rate in studies involving live performance for different pieces of
376 classical music.³⁹ In contrast to EEG, we may expect that ISC-HR is less sensitive to low-
377 level features of a stimulus. Neural evoked responses can be driven by low-level features such
378 as luminance or sound fluctuations, which can elicit strong responses that would be trivially
379 synchronized across subjects.^{19,61} To us it is less clear how such low-level stimulus fluctuations
380 could drive HR fluctuations.

381 We have shown here that the effect on HR synchronization is dominant in the frequency band
382 around 0.1Hz, which falls in the frequency range of respiratory sinus arrhythmia.⁴⁶ However,
383 we show here that breathing does not synchronize between subjects, nor is the link between
384 breathing and instantaneous heart rate dependent on attention. Given the link between
385 respiratory sinus arrhythmia and parasympathetic cardiac control,⁶² this result suggests that
386 attention does not affect parasympathetic activity.

387 Finally, we made a proof-of-concept that the ISC-HR could be used as a simple marker for
388 cognitive state in unresponsive patients. Note that this is in line with previous work on ISC of
389 EEG²⁸, fMRI³⁰, and similar findings with galvanic skin response⁶³. While we were able to
390 distinguish patients from healthy controls, we were not able to resolve conscious states among
391 patients. However, the results do suggest that the ISC-HR might carry information related to
392 the patients' recovery. Note that the proposed method requires the patients to be conscious,
393 but also to be able to process language. This double requirement may explain the positive test
394 in one patient who recovered with preserved language processing, and a negative test in a
395 patient who recovered in an aphasic condition. In addition, we believe that the 10 minutes story
396 we used may have been too short for a reliable measure of ISC-HR. In the present experiments
397 we required at least 15 minutes of instantaneous heart rate to detect significant ISC, and a link
398 to memory. We suggest that future studies on clinical utility use one or several narratives
399 totaling at least 30 minutes of concurrent heart rate recordings. In addition, our results also
400 indicate that the actual content of the story, and how engaging it is for the subject, plays a role
401 in the individual ISC. Given the limited cognitive status of the patients it is critical to maximize
402 this factor. We also suggest that the narratives should be adapted for every single patient, for
403 instance by changing the name of the leading character using the patients' own name. By doing
404 so we will amplify the patients' attention while keeping the overall structure of the story
405 comparable across subjects.

406

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559

560

561 Methods

562 Datasets

563 *Experiment 1 : auditory narratives with healthy participants*

564 Twenty-seven native English speakers and healthy participants (22 females, age range 18-
565 26, median 21 years old) listened to a 16-minute extract of an audiobook read by a male British
566 English voice (20,000 leagues under the sea. Author: Jules Verne. Read by: David Linski.
567 Public Domain (P) 2017 Blackstone Audio, Inc.) while their EKG was recorded. The audiobook
568 extract was taken from the first chapter and half of the second chapter. The text is relatively
569 suspenseful as it describes reports of an unknown monster that destroys ships. We divided
570 the story into essays of approximately 1 minute each so that participants could take breaks
571 between segments if they wished.

572 The instructions given to the subject were 'to listen to the story and look at a fixation cross'.
573 The stimuli were delivered by headphones - ER-1 Insert Earphones (Etymotic Research),
574 using Psychopy v3.1.2. The EKG was recorded with two electrodes on the chest using
575 SenseBox of ANT Neuro, sampled at 500Hz.

576 EKG data was cut into the 16 epochs of approximately 1-minute corresponding to each audio-
577 segment.

578 This study was approved by the STEM ethics committee of the University of Birmingham,
579 England.

580

581 *Experiment 2: instructional videos with healthy participants*

582 Thirty-one students watched 5 instructional videos while their EKG were recorded (19 females,
583 age range 18-46, median 28 years old) in an attentive condition (A), where they were instructed
584 to simply watch videos as they would regularly watch a video. Each educational video was 3-
585 5 minutes long, chosen from popular YouTube channels covering biology, physics, and
586 computer science. These are new recordings on videos we had tested previously.³⁵ After the
587 students had watched all 5 videos, they were asked to answer 10-12 questions about factual
588 information about material conveyed in each video. Lastly, students were instructed to watch
589 the video again in a distracted condition (D). In this condition participants were asked to silently
590 count in their mind backwards from a random prime number above 800 and below 1000, in
591 steps of 7.

592

593 The experiment was carried out at the City College of New York in a sound-attenuated booth.
594 Subject wore headphones and watched the videos on a 19" monitor. The EKG was recorded
595 with a BioSemi Active Two system at a sampling frequency of 2048Hz. 2 EKG electrodes were
596 placed below the left collar bone and one on the left lumbar region. For segmentation of the
597 EKG signal onset and offset triggers were used, in addition a flash and beep sound was
598 embedded right before and after each video which were recorded using a StimTracker
599 (Cedrus) to ensure precise alignment across all subjects. Of the thirty-one participants 4 were
600 removed from analysis due to bad signal quality resulting in usable data for N=27 participants.

601 The experimental protocol was approved by the Institutional Review Boards of the City
602 University of New York. Documented informed consent was obtained from all subjects for
603 laboratory experiments.

604

605 *Experiment 3: auditory narratives with healthy participants and respiration*

606 The EKG of 25 french native healthy participants (15 females; age range 22-28, median age
607 25 years old) listened to four stories while their EKG and respiration was recorded using a
608 Polygraph Input Box (PIB of EGI-Geodesic's physiological measurement system). This
609 includes a chest belt to measure respiratory movement (Respiration Belt MR - Brain Products)
610 and 2 EKG electrodes placed on the left subclavicular area and below the left axillary area. Of
611 the twenty-five participants four were removed because of missing respiratory and/or cardiac
612 data. The four audio stimuli come from <https://www.franceinter.fr/emissions/une-histoire-et-oli>
613 : (1) Nadine et Robert les poissons rouges- Delphine de Vigan (8 min) (2) les villages du
614 versant – Alice Zeniter (8 min) (3) Opaque et Opaline - Alex Vizorek (11 min) (4) le renard et
615 le poulailler – Guillaume Meurice (10 min).

616 To test whether the ISC-HR is modulated by attention we divided the subjects into 2 groups:
617 Group 1 (9 subjects) was recorded with stories (1) and (2) in a distracted condition, and (3)
618 and (4) in an attentional condition. In group 2 (12 subjects) the stories were counterbalanced,
619 stories (1) and (2) in the attentional condition, and (3) and (4) in the distracted condition. In the
620 attentional condition (A), the subject's task was to pay attention to the story while disregarding
621 tones (320/360/400/440/482 Hz, 400ms long) that were played in random intervals (between
622 800ms and 1100ms) in the background of the story. After each story the subjects received a
623 control debriefing questionnaire including 5 questions testing the memory performance of the
624 story content. In the distracted condition (D), the subject's task was to count backwards starting
625 from 100 indexing the occurrence of 'counting' tones (same tones as in the attentional
626 condition) in-between 2 'reset' tones (Audacity- the type of tones is a linear decay between
627 1300 and 400 Hz during 400ms). The reset tones were added uniformly and randomly every
628 14 seconds on average. After each 'reset' tone, subjects had to reset the counting back to 100.
629 At the end of the block the subjects had to report the smallest number obtained between 2
630 'reset' tones. Subjects were instructed not to pay attention to the story and also receive the
631 same debriefing questionnaire. The present research was promoted by the Inserm (CPP C13-
632 41) and approved by the Comité de Protection des Personnes Ile-de-France 6. All subjects
633 provided written informed consent.

634 *Experiment 4: Auditory narratives with disorder of consciousness patients and healthy controls*

635 Nineteen patients (8 females, age range 18 to 77, median age 50 years old) with disorders of
636 consciousness (mostly resulting from brain lesions) and 24 healthy control subjects (14
637 females; age range 23-27, median 25 years old) listened to an auditory narrative (La part des
638 ancêtres - Leonora Miano - 10 minutes, from: [https://www.franceinter.fr/emissions/une-](https://www.franceinter.fr/emissions/une-histoire-et-oli)
639 [histoire-et-oli](https://www.franceinter.fr/emissions/une-histoire-et-oli)) through headphones while their EKG was recorded with a Polygraph Input Box
640 (PIB of EGI-Geodesic's physiological measurement system). The only instruction given to all
641 subjects (healthy controls and patients) was to listen to the story. These patients were
642 hospitalized in neurointensive care at Pitié Salpêtrière (medical center with expertise in
643 disorder of consciousness) to determine their state of consciousness, to adapt treatment, and
644 to evaluate their neurological prognosis. During this evaluation, we performed several exams:
645 clinical assessment, MRI, EEG, evoked response potential, and positron emission
646 tomography. The state of consciousness is determined with some⁶¹ behavioral assessments,

647 using the Coma Recovery Scale-revised⁴³ - a score which allows differentiating between
648 consciousness states: Coma (the patient does not open their eyes), Vegetative State (VS -
649 Eye-opening, and alternance between wakefulness and sleep), Minimally Conscious State
650 (MCS - the patient is able to follow their own face in the mirror or to follow a simple instruction)
651 and Exit Minimally Conscious State (EMCS - patient can communicate with code). Among the
652 19 patients, we diagnosed 2 patients in coma, 8 VS patients, 8 MCS patients (7 MCS- and 1
653 MCS+) and 1 EMCS (see supplementary data for more details). The Ethical Committee of the
654 Pitie-Salpetriere approved this research under the French label of 'routine care research'.

655 **Computation of intersubject correlation of heart rate (ISC-HR)**

656 Previous studies have relied on the quantification of synchrony of neuroimaging based time
657 series (i.e. BOLD in fMRI²⁵ or signals from EEG electrodes²⁷). We follow a similar logic for
658 the electrocardiographic (EKG) signal. We focus on the modulation of heart rate, by doing so
659 we can determine if subjects increase or decrease their heart rate simultaneously,
660 independently of their absolute level of heart rate. Step 1: We measure the EKG signal and
661 detrend it using a high-pass filter (0.5 Hz cutoff) and subsequently notch filtered at either 50Hz
662 (Experiment 1, 3 and 4) or 60 Hz (Experiment 2). We compute the instantaneous HR by
663 detecting RR intervals from the EKG (Figure 1A). Peaks of the R-wave were found using
664 *findpeaks* (built-in matlab function). Step 2: The instantaneous HR signal is then interpolated
665 to keep the same sampling frequency for all subjects (Figure 1B). Step 3: This interpolated
666 instantaneous HR signal is used to compute an inter-subject correlation matrix by calculating
667 the Pearson's correlation between each subjects' instantaneous HR signal (Figure 1C). Step
668 4: Finally, the intersubject subject correlation of heart rate (ISC-HR) for each subject is obtained
669 by computing the mean of correlations of that given subject to the rest of the group (Figure
670 1D).

671 For Experiment 2 (Fig 3. and 4) in step 3 we computed the inter-subject correlation matrix
672 between the instantaneous HR signals in the attentive and distracted conditions with the
673 instantaneous HR in the attentive conditions rather than within condition. In Experiment 3 (Fig.
674 5) we again used the instantaneous HR signals obtained when the groups were attentively
675 listening to the stories as reference when computing the inter-subject correlation matrix for step
676 3 (Fig. 6.). For Experiment 4 we used the healthy participants as reference in the computation
677 of the inter-subject correlation matrix in step 3. All other steps were as explained above.

678 **Statistical significance of ISC-HR**

679 The instantaneous HR signals for a given epoch are first aligned across subjects. Then ISC-
680 HR was calculated for all subjects in all epochs and the ISC across epochs. To test whether
681 the ISC-HR value for each epoch was statistically significant (for Fig. 2A), circular shuffle
682 statistic was used: Each subject's instantaneous HR is circularly shifted by a random amount
683 within the 60 second segments and the ISC-HR is re-computed. This procedure is repeated
684 10.000 times and the ISC-HR of the epoch is compared to this distribution of ISC-HR values
685 for the circular shifted instantaneous HR signals. The p-value is obtained by counting how
686 many circular shifted ISC-HR values were below the actual ISC-HR value. For Fig. 2B we
687 repeat the circular shift to compute ISC-HR values and then average across epochs; p-values
688 are then computed on these averaged ISC-HR values. For Figure 2C, instead of circular shifts
689 within 60 s story segments, we instead randomly swapped segments between participants.

690

691 **Frequency analysis of heart rate fluctuations**

692 To investigate which time scale the inter-subject correlation and HRV is modulated by attention
693 we do a frequency analysis of the instantaneous HR signal (Figure 4). The instantaneous HR
694 signal was band-pass filtered using 5th order butterworth filters with logarithmic spaced center
695 frequencies with a bandwidth of 0.2 of the center frequency. The ISC was computed in each
696 frequency band referenced to the attentive group (Fig. 4A). The HRV was computed as the
697 standard deviation of the instantaneous HR normalized with the average HR (Fig. 4B).

698 **Computation of Fractional Anisotropy index (FA index)**

699 Diffusion Tensor Images (DTI) were acquired on a 3T Siemens Skyra scanner (64 diffusion
700 gradient directions, b value = 1000 s/mm², TR/TE = 3000/80 ms, voxel size = 2x2x2 mm³).
701 DTI data were pre-processed using the FDT package from the Functional MRI of the Brain
702 (FMRIB) software library (FSL) package 5.01⁶⁴. This consisted of: 1) correcting for motion and
703 distortions caused by eddy currents; 2) brain segmentation using the brain extraction tool
704 algorithm; 3) computing the fractional anisotropy (FA) maps using the diffusion-tensor model;
705 4) registration of the FA and MD maps on the FA template in the standard Montreal
706 Neurological Institute (MNI) space using linear as well as nonlinear spatial transformations.
707 FA values were averaged within a deep white-matter mask defined in the MNI space as the
708 outline of the ICBM-DTI-81 white-matter labels atlas⁶⁵. For each subject, this FA value was
709 normalised with the mean of FA values measured from 10 healthy volunteers acquired with
710 the same imaging protocol, such that an average FA index of 1.0 can be considered normal.
711

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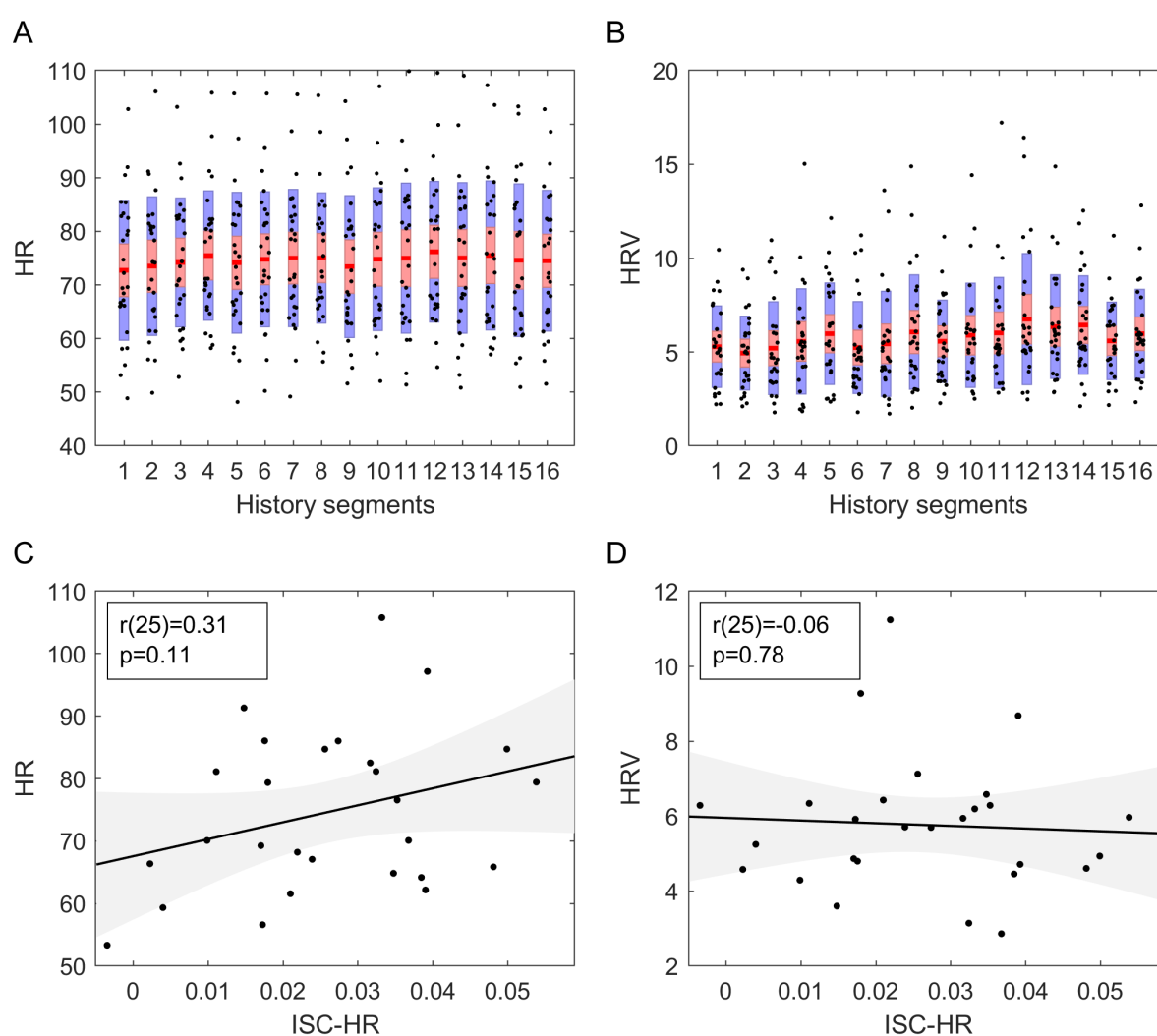
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719

720

721 Supplementary materials

722 Analysis of mean HR and HRV for experiment 1

723 For experiment 1 we also checked whether mean HR or HR variability (HRV) differed between
724 story segments or between subjects (Fig. S1A and S1B). ANOVA with segment as fixed effect
725 and subject as random effects shows that mean and standard deviation of HR differed between
726 segments (HR: $F(15,390)=2.46$, $p=1.89e-03$, HRV: $F(15,390)=1.73$, $p=4.26e-02$), and between
727 subjects (HR: $F(26,390)=316.92$, $p=2.93e-244$, HRV: $F(26,390)=13.52$, $p=4.92e-40$). We did
728 not see a relationship between HR-ISC and mean HR (Fig. S1C, $r(25)=0.31$, $p=0.11$), or
729 between HR-ISC and HRV (Fig. S1D, $r(25)=-0.06$, $p=0.78$).



730 **Supplementary Figure 1:** **A:** The instantaneous heart rate shows no modulation across
731 epochs (Anova $F(15,390) = 1.04$, $p = 0.41$), but differences across subjects (Anova
732 $F(26,390)=173.88$, $p=0$). **B:** Heart rate variability measured as the standard deviation across
733 the instantaneous heart rate for each segment.
734 **C:** ISC-HR for each subject averaged across segments versus corresponding mean HR (each
735 subject is a dot). We found no linear relationship between these two variables.
736

737 **D:** ISC-HR for each subject averaged across segments versus corresponding HR variability
738 (each subject is a dot). We found no linear relationship between these two variables.

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740

741 **Analysis of mean HR and HRV for experiment 2**

742 For experiment 2, in addition to the attentional effects reported in the main results section, we
743 also checked whether mean HR or HR variability differed between each educational video and
744 between subjects (Fig. S2A and S2B). ANOVA with video as fixed effect and subject as random
745 effects shows that mean HR differed across videos (HR: $F(4,211)=3.05$, $p=1.81e-02$), but not
746 standard deviation ($F(4,211)=0.77$, $p=5.44e-01$), and both differed significantly between
747 subjects (HR: $F(23,211)=89.19$, $p=1.87e-95$, HRV: $F(23,211)=29.56$, $p=1.57e-53$). We did not
748 see a relationship between ISC-HR and mean HR (Fig. S2C, Attentive: $r(25)=-0.16$, $p=0.43$,
749 Distracted: $r(25)=0.21$, $p=0.29$) or between ISC-HR and HRV (Fig. S2D, Attentive: $r(22)=0.15$,
750 $p=0.48$, Distracted: $r(22)=0.21$, $p=0.46$).

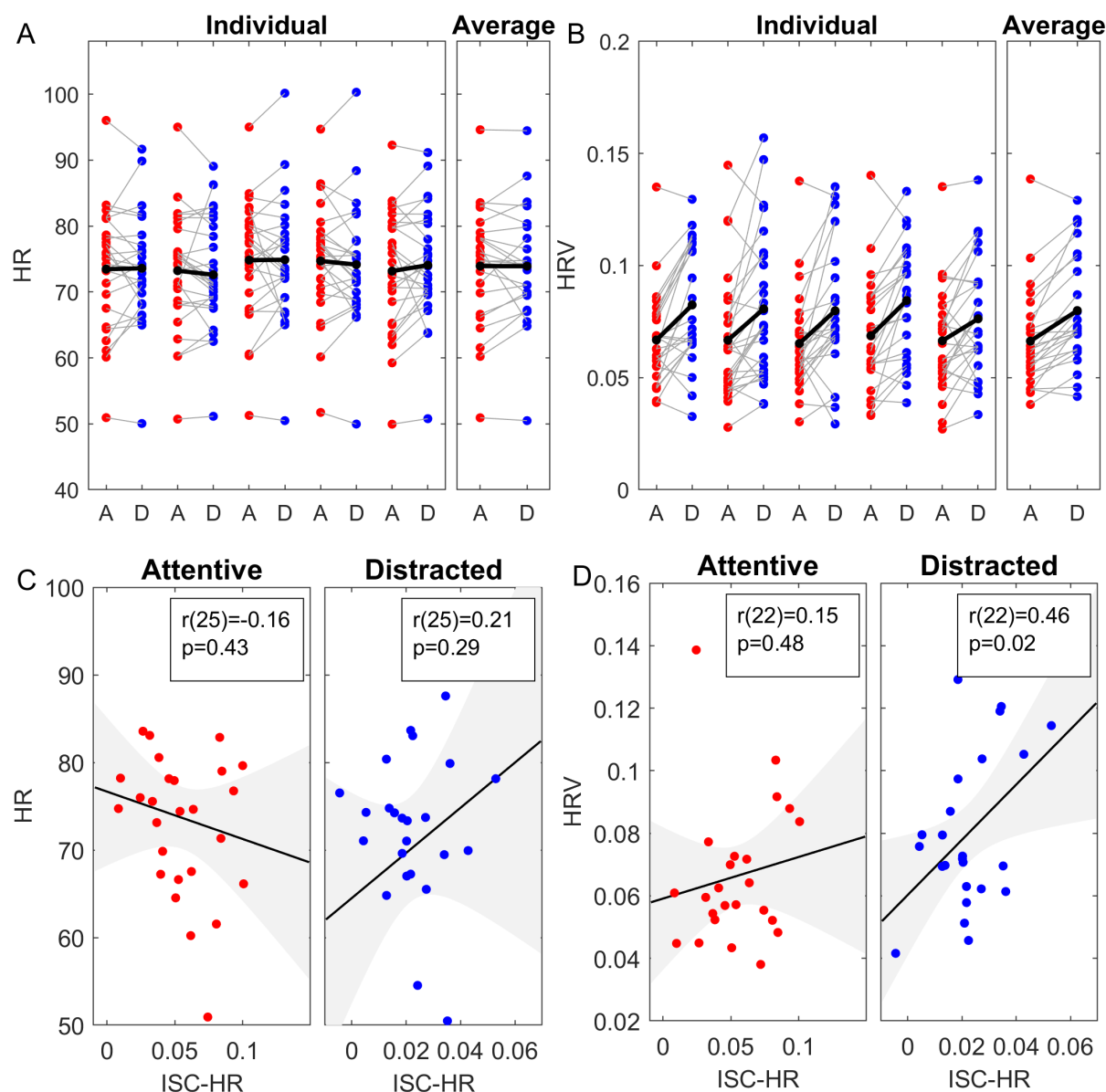
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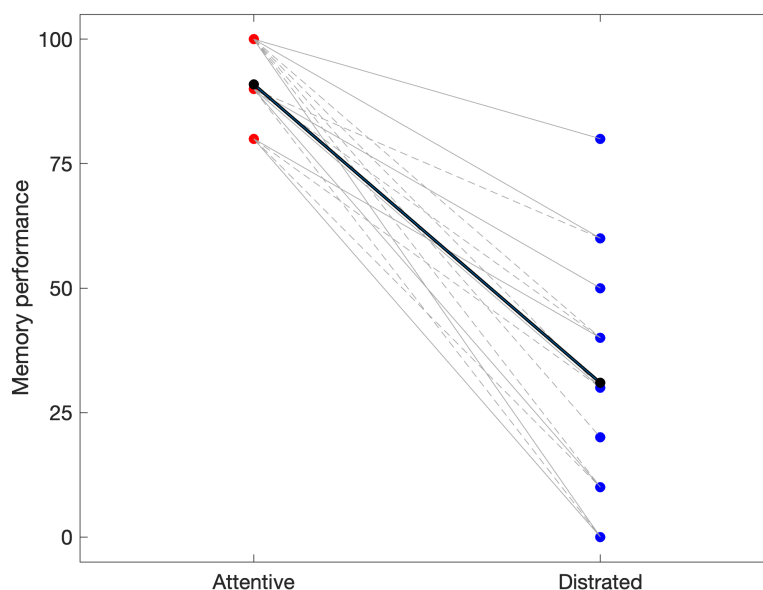
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Supplementary figure 2: A: mean HR, **B:** HRV, **C:** correlation of ISC with HR. **D:** correlation of ISC with HRV

761 Behavioral results of experiment 3

762 For experiment 3, we checked the modulation of memory performance in the attentive and
763 distracted condition like a proof that the task was correctly completed. After each story,
764 subjects answered 5 short questions about the story content testing their memory performance
765 (i.e name of protagonist?, place?...). Memory performance was significantly higher in the
766 attentive condition than in the distracted condition (Figure S3, Wilcoxon signed-rank test: $z =$
767 4.03 , $p = 5.6789e-05$). In none of the conditions we found a difference between group 1 and 2
768 in terms of memory performance. In both groups the performance was always similar, in the
769 attentive condition (Median group 1 = 90; Median group 2 = 90; Mann-Whitney U test, $U = 93$,
770 $p = 0.67$), in the distracted condition (Median group 1 = 40; Median group 2 = 30; Mann-Whitney
771 U test, $U = 106$, $p = 0.66$), or in the contrast between the attentive and distracted conditions
772 (Median group 1 = 40; Median group 2 = 65; Mann-Whitney U test, $U = 86.5$, $p = 0.39$)

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776 **Supplementary figure 3: Behavioral responses attentive and distracted conditions (n=21).** Solid
777 lines correspond to subjects in group 1 and dashed lines to subjects in group 2. Each group listened to
778 2 two stories in the attentive condition and two in the distracted condition.

779 Subjects answered 5 short questions about each story content. The memory performance (rate of good
780 response) was systematically higher in the attentive condition compared to the distracted conditions.

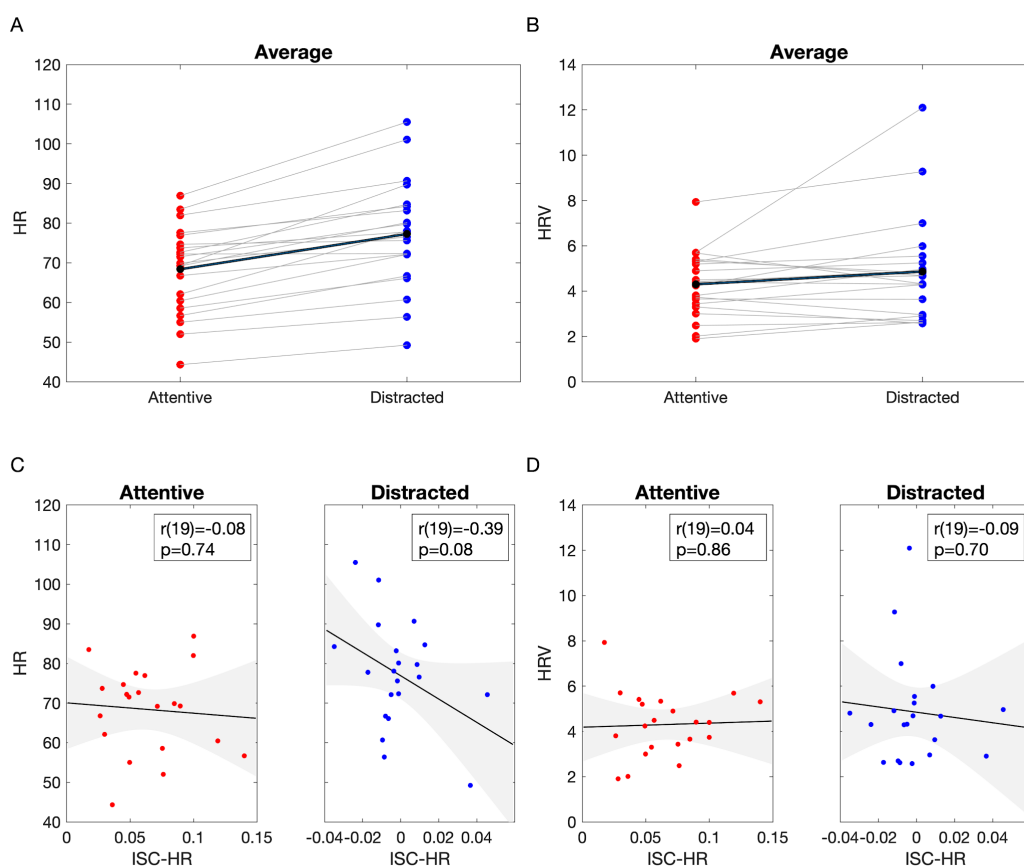
781 We observed no differences in memory performance between groups.

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783 **Analysis of mean HR and HRV for experiment 3**

784 For experiment 3 we also checked whether mean HR or HR variability differed between each
785 condition and between subjects. We found that the mean HR was significantly higher in the
786 distracted condition compared to the attentive condition (Fig S4A, paired t-test, $t(21) = 7.32$, p
787 $= 4.5e-7$). We found no differences in HRV between the attentive and distracted conditions
788 (Fig S4B, paired t-test, $t(21) = 1.64$, $p = 0.12$).

789 We also did not see a relationship between ISC-HR and mean HR (Fig. S4C, Attentive: $r(19)=-$
790 0.08 , $p=0.74$, Distracted: $r(19)=-0.39$, $p=0.08$) or between ISC-HR and HRV (Fig. S3D,
791 Attentive: $r(19)=0.04$, $p=0.86$, Distracted: $r(19)=-0.09$, $p=0.70$).



792

793 **Supplementary figure 4: A:** mean HR, **B:** HRV, **C:** correlation of ISC with HR in the attentive
794 condition (left), and distracted condition (right), **D:** correlation of ISC with HRV in the attentive
795 condition (left), and distracted condition (right)

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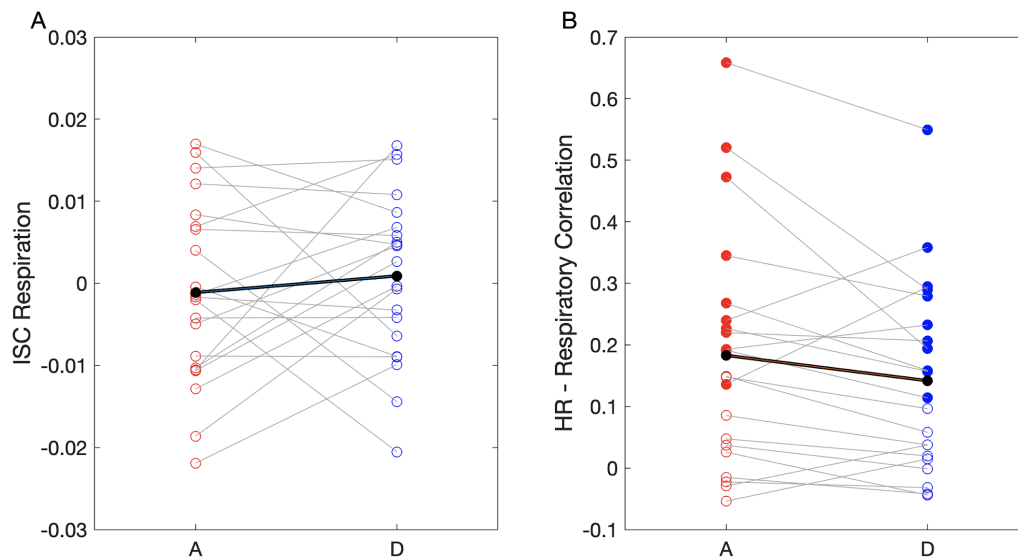
811 **Respiration and HR and for experiment 3**

812 Breathing is known to be a determinant of the heart rate. We checked whether the
813 synchronization of respiration between subjects was modulated by the attentive/distracted
814 conditions. We showed no difference of ISC respiration between both conditions (Fig S5A,

815 paired t-test, $t(21)=0.5$, $p=0.6$), in addition none of the subjects had significant individual ISC
816 value in either condition.

817 However, we tested if breathing cycle correlates with HR for each subject (Individual Pearson
818 correlation between displacement of the chest sensor and instantaneous HR), and if this
819 correlation is modulated by the attentional condition (Fig. S5B). The phase of breathing cycle
820 and HR were significantly correlated (one-sample t-test averaging the coupling of each
821 individual in the attentive and distracted conditions, $t(20)=4.49$, $p=2e-4$). However, the
822 difference in coupling between the attentive and distracted conditions did not reach significance
823 (paired t-test between attentive and distracted conditions: $t(20)=1.86$, $p=0.08$). Permutation
824 tests, shuffling the temporal relationship between HR and respiration time-series of each
825 individual indicated that 11 out of the 21 subjects (both in the attentive and distracted
826 conditions) showed individually significant HR-Respiratory correlation (FDR corrected, p
827 <0.01).

828



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831 **Supplementary figure 5:** (A) ISC of respiration shows no significant changes of ISC between
832 attentive and distractive conditions. (B) HR-Respiratory cycle coupling was significant for each
833 subject represented by the filled circles ($p < 0.005$), attention and distractive conditions did not
834 modulate the HR-Respiratory cycle coupling (paired t-test: $t(20)=1.86$, $p=0.08$).

835 Filled and empty circles indicate subject-level significant and non-significant respectively (FDR
836 $p < 0.01$ permutation statistics, shuffling the temporal relationship between HR and respiration
837 time-series)

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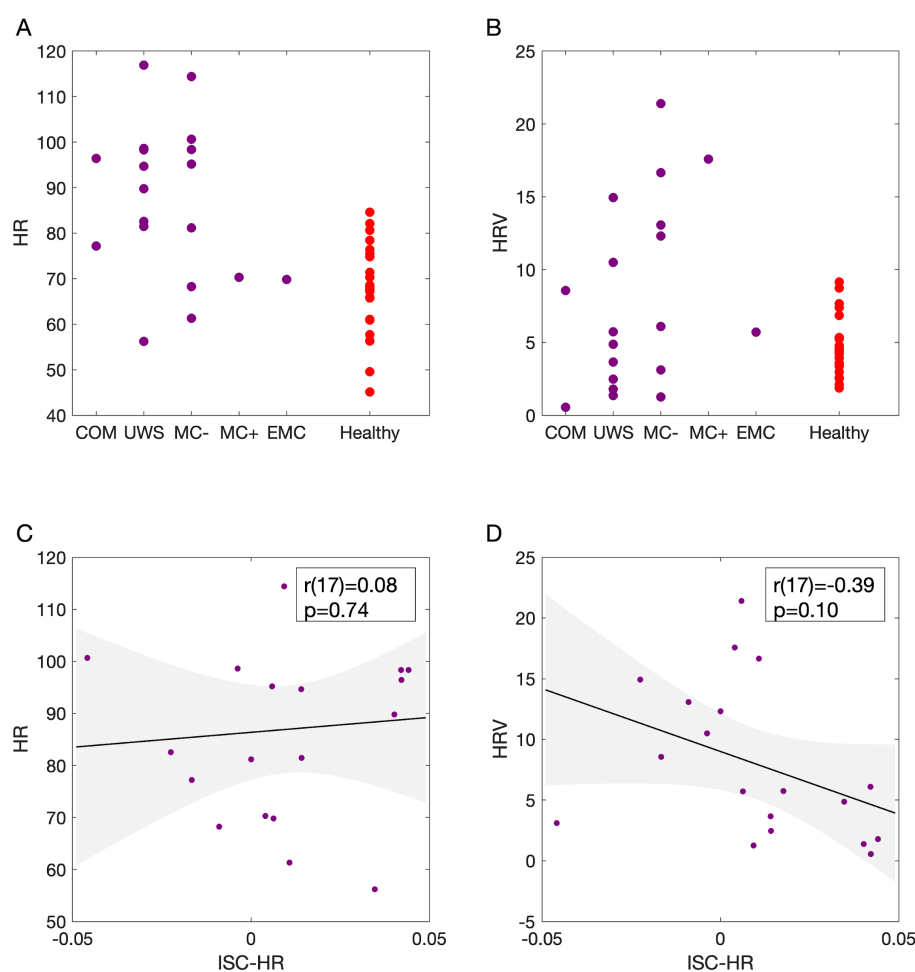
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840 **Analysis of mean HR and HRV for experiment 4**

841 For experiment 4 we also checked whether mean HR or HR variability differed between the
842 different states of consciousness (Fig. S6). The mean HR of DoC patients was significantly
843 higher than healthy participants (Fig S6A, $t(41) = 4.7$, $p = 2.9e-05$). To test if HR changed with

844 the state-of-consciousness among the DoC patients we performed a Spearman correlation
845 between state-of-consciousness (Coma = 1, VS = 2, MCS- = 2, MCS+ = 3, EMCS = 4) and HR
846 and found no significant correlation ($R(17) = -0.18$, $p = 0.45$). Similar for the HR variability, HRV
847 was significantly higher in DoC patients compared to healthy controls (Fig S6B, $t(41) = 2.34$, p
848 $= 0.02$). We found no significant relationship between the patients' state-of-consciousness and
849 HRV (Spearman correlation, $R(17) = 0.41$, $p = 0.08$).

850 We also controlled the relationships between HR and ISC, and HRV and ISC for patients. In
851 none of the cases the relationship was significant (Fig. S6C, HR versus ISC, $r(17)=0.08$,
852 $p=0.74$; Fig. S6D, $r(17)=-0.4$, $p=0.09$).



853

854 **Supplementary figure 6: A:** mean HR for DoC patients and healthy participants (Note that
855 DoC patients are ordered in individual columns corresponding to their clinical state-of-
856 consciousness (1=Coma, 2=VS/UWS, 3=MCS-, 4=MCS+, and 5=EMCS) **B:** HRV, idem to A
857 **C:** correlation of ISC with HR for DoC patients. **D:** correlation of ISC with HRV for DOC patients.

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| Subject | Sex | Age (years) | Etiology | Delay (days) | State | CRS-R | FA | Outcome |
|---------|-----|-------------|----------------------------|--------------|-------|-------|------------|-----------|
| 1 | M | 71 | Acute Polyradiculoneuritis | 12 | Coma | 0 | no exam | VS/Death* |
| 2 | F | 77 | Meningitis | 86 | Coma | 2 | no exam | VS |
| 3 | M | 18 | TBI+Anoxia | 170 | VS | 5 | 0.756 | VS |
| 4 | M | 29 | TBI+Anoxia | 510 | VS | 5 | artefacted | VS |
| 5 | M | 29 | Anoxia | 556 | VS | 5 | 0.492 | VS |
| 6 | M | 55 | TBI | 27 | VS | 6 | artefacted | MCS+ |
| 7 | F | 53 | Anoxia | 328 | VS | 5 | 0.824 | VS |
| 8 | F | 24 | TBI | 68 | VS | 5 | 0.644 | MCS- |
| 9 | F | 63 | Anoxia | 41 | VS | 5 | 0.642 | VS |
| 10 | M | 18 | Anoxia | 59 | VS | 4 | 0.792 | VS/Death* |
| 11 | F | 50 | Anoxia | 5852 | MCS- | 10 | 0.698 | MCS- |
| 12 | M | 26 | Status Epilepticus | 209 | MCS- | 9 | 0.561 | MCS+ |
| 13 | M | 50 | Anoxia | 60 | MCS- | 7 | 0.85 | EMCS |
| 14 | F | 61 | Status Epilepticus | 90 | MCS- | 10 | noDTI | MCS- |
| 15 | M | 58 | Anoxia | 302 | MCS- | 14 | 0.548 | MCS- |
| 16 | M | 56 | TBI | 478 | MCS- | 11 | 0.824 | MCS-* |
| 17 | F | 36 | Left hematoma | 121 | MCS- | 12 | noDTI | EMCS |
| 18 | F | 49 | TBI | 980 | MCS+ | 13 | noDTI | MCS+ |
| 19 | M | 28 | Status Epilepticus | 313 | EMCS | 14 | no exam | EMCS |

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864 **Description of patient cohort:** summary table including patients with sex, age, etiology of
 865 brain lesion, delay between brain lesion and the evaluation, state of consciousness, CRS-R
 866 (Coma Recovery Scale-Revised), Fractional anisotropy (FA) from MRI and outcome.
 867 *Outcome collected before 6 months.

868