A neuromechanical model for *Drosophila* larval crawling based on physical measurements

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Short title: A neuromechanical model for fly larval crawling

Abstract

Animal locomotion requires dynamic interactions between neural circuits, muscles,

and surrounding environments. In contrast to intensive studies on neural circuits, the

neuromechanical basis for animal behaviour remains unclear due to the lack of information

on the physical properties of animals. Here, we proposed an integrated neuromechanical

model based on physical measurements by taking *Drosophila* larvae as a model of soft-

bodied animals. The biomechanical parameters of fly larvae were measured by the stress-

relaxation test. By optimizing parameters in the neural circuit, our neuromechanical model

succeeded in quantitatively reproducing the kinematics of larval locomotion that were

obtained experimentally. This model could reproduce the observation of optogenetic studies

reported previously. The model predicted that peristaltic locomotion could be exhibited in a

low friction condition. Analysis of floating larvae provided results consistent with this

prediction. Furthermore, the model predicted a significant contribution of intersegmental

connections in the central nervous system, which contrasts with a previous study. This

hypothesis allowed us to make a testable prediction for the variability in intersegmental

connection in sister species of the genus *Drosophila*. Our model based on physical

measurement provides a new foundation to study locomotion in soft-bodied animals and soft

robot engineering.

Introduction

Animal behaviour requires both neural circuits and the body. Specific neural circuits

referred to as central pattern generators (CPGs) are capable of creating spatiotemporal

activity patterns for behaviours (1–5). CPGs regulate motor neuron activity and muscular

contraction to generate force for movement. On the other hand, the body's physical

properties and constraints are also significant factors to guarantee animal movements (6–9).

Accordingly, integration of neural circuits and body mechanics, referred to as

neuromechanics, is one of the essential approaches to reveal motor control mechanisms

(10–15).

Soft-bodied animals locomote by deforming their stretchable bodies (16). Compared

to animals with hard skeletons, soft-bodied animals possess high flexibility and can move

adaptively in complicated environments (17). This flexibility of soft-bodied animals suggests

that output from neural circuits is not the sole determinant for locomotion. Animal's physical

properties such as stiffness and viscosity should also be involved in the dynamics of

locomotion (9,15) and have been measured experimentally (18–23). However, it is still

challenging to reproduce locomotion in soft-bodied animals by mathematical models based

on physical measurements. To tackle this issue, we used *Drosophila melanogaster*

(*Drosophila*, hereafter) larvae as a model and attempted to build a neuromechanical model

describing their crawling behaviour.

Forward crawling is the most predominant mode in fly larval locomotion (24,25). By

propagating segmental contraction from the posterior to anterior segments, larvae move

forward (26–28), and neural circuits for crawling have been intensively examined (29–37).

Previous simulation studies have succeeded in building models describing the propagative

nature of crawling behaviour qualitatively (10,38–40). In contrast, the physical properties of

larvae remained to be studied, and quantitative reproduction of crawling kinematics has not

been achieved yet.

Here, we present a neuromechanical model to describe fly larval crawling behaviour

based on their locomotion kinematics and soft-bodied biomechanics. First, we recorded

forward crawling in the third-instar larvae whose segmental boundaries were labelled by a

fluorescent protein and extracted kinematics parameters of crawling. Then using a tensile

tester combined with optogenetics, we measured larval contraction force. Furthermore, larval

viscoelasticity was measured by the tensile tester. The measurement indicated that the

properties of the larval body were described better by the standard linear solid (SLS) model

than the Kelvin-Voigt model previously used (10,41). By incorporating these physical

parameters with a neural circuit model built previously (10), we established a

neuromechanical model for larval locomotion. By optimizing the neural circuit model

parameters, we succeeded in building a neuromechanical model that reproduced the

kinematics parameter extracted from larva measurements. This model could also reproduce

optogenetic studies reported previously. In addition, crawling in a low friction condition was

simulated, and its prediction was confirmed experimentally by analyzing floating larvae.

Perturbation analyses in our model predicted the importance of intersegmental connections

in speed control, contrasting to previous studies (10,40). Based on our simulation results, we

predicted the intersegmental connectivity in sister species in the genus *Drosophila*. Our

model for larval crawling based on physical measurements provides a new approach to

locomotion research in soft-bodied animals and soft robot engineering.

Results

Measurement of forward crawling behaviour in third-instar larvae

To reveal the physical mechanisms behind *Drosophila* larval crawling, we examined

the kinematics of the behaviour and physical properties of the body. We used third-instar

larvae because their size (3.53 ± 0.12 mm, n = 9 larvae) was large enough to measure

physical properties as a soft material. While previous studies examined first- or second- instar

Drosophila larvae and characterized the segmental kinematics (26,27,37,42,43), crawling

behaviour in the third-instar larvae had not been investigated at a segmental scale but

instead at a scale of the entire body (24,25,28,32,44). Thus, we examined the segmental

dynamics in freely moving third-instar larvae.

First, we recorded the position of the segment boundaries in freely crawling larvae.

To reliably trace the segmental boundaries of larvae, we expressed a GFP-tagged

coagulation protein Fondue, which accumulates at the muscle attachment sites (45). We

acquired time-lapse fluorescence images from the dorsal side of the larvae where

longitudinal muscles span single segments (Figure 1A). From these fluorescence images,

the segmental boundaries of the thoracic (T2-T3) and abdominal (A1-A8) segments were

annotated (Figure 1B. See Materials and Methods for details.) We examined the

displacement of each segment boundary during forward crawling. As previously reported in

the first- and second-instar larvae cases, sequential displacement of the segmental boundary

from the posterior to anterior segments was observed in third-instar larvae (Figure 1C). Four

kinematic parameters were measured from the recording: Stride length, stride duration,

intersegmental delay, and speed (Figure 1D). We obtained that stride length was 0.70 ± 0.05

mm, stride duration was 1.07 ± 0.12 sec, intersegmental delay was 0.09 ± 0.01 sec, and

speed was 0.64 ± 0.02 mm/sec (n = 9 larvae).

Next, we quantified the dynamics of segmental length change. Plots of the segmental

length showed the propagation of segmental contraction in crawling larvae (Figure 1E and

1F). We measured three kinematic parameters (maximum segment length, minimum

segment length, and contraction duration described in Figure 1G) and obtained that

maximum segmental length was 0.41 ± 0.03 mm, minimum segmental length was $0.21 \pm$

0.02 mm, and contraction duration was 0.44 ± 0.03 sec (n = 9 larvae). To sum, we measured

the seven kinematics quantities from segmental dynamics in freely crawling GFP-labelled

third-instar larvae.

Consistent kinematic properties among segments in larval crawling

To establish a mathematical model for larval crawling, we examined whether we

could assume that all the segments possess similar kinematic properties or not. To this aim,

we compared the dynamics of segmental length change (defined in Figure 1G) among all the

segments (Figure 2A-2C). We noticed that the most posterior A8 segment had a shorter

maximum length and smaller contraction range than the other segments (Figure 2B). This

observation reflected the fact that the A8 segment was a specialized structure and different

from the others in the surface area of the body wall and the number of muscles (46). In

contrast, in the other segments, both the minimum and maximum lengths were comparable

over the segments. (Figure 2B). Furthermore, contraction duration was also similar among

the segments from T2 to A7 (Figure 2C). Accordingly, most segments (T2-A7) exhibited

similar kinematic dynamics in contraction during crawling, which allowed us to model the

larva as a chain of segments with the same kinematic properties.

Having confirmed the similarity among the body segments, we inferred the effective

number of segments. First, we adapted a segment model based on the "piston phase" of

larval peristalsis, where the motion of the head and tail were coupled (10,26). When a

peristaltic wave reached the head, the tail was forced to move forward, which induced the

contraction of the posterior segment A8 for the next stride of crawling. Then, we estimated

the effective number of segments by assuming that the displacement of the virtual anterior

end was the same as that of the tail. To evaluate the propagation velocity, we obtained

intersegmental delay by calculating the cross-correlation of displacements between the most

posterior segment boundary (y10) and the other segments (y0-y9) (Figure 2D). The graph

showed the propagation of segmental contraction from the posterior to the anterior segment.

By plotting the intersegmental delay normalized by the stride duration, we noticed that the

segmental contraction propagates at about a constant speed (Figure 2E). This observation

allowed us to model the larval crawling as the propagation of segmental contraction at a

uniform speed. Based on this assumption, we inferred the effective number of segments of

the whole body where the head and tail were coupled. To this aim, we fitted the

intersegmental delay data by linear regression. The intersection points between the fitting

lines and the line that the normalized intersegmental delay equalled one corresponded to the

event when the propagation of segmental contraction reached the anterior end and the

subsequent propagation was initiated. From this calculation, we obtained 11.2 ± 0.2 as the

effective number of segments (Figure 2F). Accordingly, the results indicated that the crawling

larva could be modelled by a chain of 11 identical segments (Supplementary Figure 1).

Measurement of larval contraction force

To establish a quantitative physical model for larval crawling, we attempted to

measure contraction force and soft material properties of larvae which enabled us to derive

a Newtonian description of crawling by linking force to motion. We measured contraction

force with the tensile tester (Figure 3A). The tensile tester allowed us to measure and control

both strain and stress of a sample material. We hooked an intact larva with insect pins and

loaded it to the tensile tester. We measured the spontaneous contraction force in larvae and

obtained values ranging from 1.4 mN to 2.7 mN (n=11 spontaneous contraction events by

three larvae, Figure 3B and 3E). Although these values reflected the range of spontaneous

contraction force, the larvae could not exhibit crawling locomotion during the measurement

since their head and tail were hooked. Accordingly, we instead attempted to measure the

maximum force that larvae could generate for crawling. To this aim, we adapted optogenetics

to activate motor neurons reliably (Figure 3C). We expressed a light-sensitive cation channel

protein Channelrhodopsin2 (47) in all of the larval type-I motor neurons (48) and illuminated

each larva with blue light (455 nm, 5.7 nW/mm2) to induce the contraction of all the body wall

muscles. Since we needed muscular force evoked by the CNS, we expressed

Channelrhodopsin2 in motor neurons instead of muscles. The contraction force

measurement with the optogenetic activation showed that the force ranged from 1.6 mN to

6.7 mN (n=44 optogenetic stimulations applied to seven larvae, Figure 3D and 3E). The

variation in the measurement would be caused by differences in some uncontrollable

conditions, including hooking states at the head and tail. Consequently, we adapted the

maximum measured force of 6.7 mN as the maximum force (F_{Mmax}) used in our

neuromechanical model.

Measurement of elastic and damping properties of larvae

Next, we analysed passive properties of the larval body, elasticity and viscosity, with

the tensile tester (Figure 4A). The stretchable body wall and hydrostatic skeleton of fruit fly

larvae were typical components in soft-bodied organisms (49). Previous studies reported

material properties of soft-bodied animals, including the caterpillar *Manduca sexta* (18) and

the earthworm *Lumbricus terrestris* (50,51). Although previous theoretical analyses of fly

larval locomotion assumed that each segment was equivalent to a pair of a spring (a linear

elastic component) and a damper (a linear viscous component) (10,39,41), mechanical

properties of *Drosophila* larvae were not measured experimentally. Accordingly, we

measured the viscoelastic properties of fly larvae by methods used in material science.

First, we analysed the range of extension within which we could assume linearity

between the extension and tensile force of the larval body (Figure 4B). To analyse the

relationship between the extension and tensile force of larvae, we stretched larvae at a

constant speed (Figure 4C) and plotted tensile force against the extension (Figure 4D). To

test the linearity, we used linear regression. Depending on the range of extension, goodness

of fitting varies: Linear regression fitted better in the range from 0 mm to 0.4 mm extension

(Figure 4E left) than in a longer range from 0 mm to 1.0 mm (Figure 4E right). To find a

suitable extension range with good linearity, we calculated the coefficient of determinants,

which was an indicator of predictability of the data by linear regression (Figure 4F). The plot

showed that extension up to 0.4 mm or 0.6 mm exhibits high coefficients. Based on this

observation, we concluded that we could assume linearity in the stretch ranging from 0 mm

to 0.6 mm.

Next, we measured the viscoelasticity of larvae. Viscoelastic properties of soft

materials could be acquired by measuring the relationship between stress (force loaded in

the material) and strain (deformation of the material) (52). To obtain the viscoelastic

properties of larvae, we conducted the stress relaxation test, one of the standard dynamic

mechanical tests (52). In this test, a soft material sample was quickly extended to a certain

length, and then the stress was being recorded over time (Figure 4G). Based on the linearity

test above, we extended third instar larvae by 0.4 mm. The result of the stress relaxation test

showed an exponential decay that was approaching a non-zero plateau at a later time (Figure

4H left). To extract physical properties from the stress relaxation data, a suitable physical

model to describe the larval body was required. Among general mechanical structure models

of linear combinations of springs and dampers, we found that the Maxwell model and the

Kelvin-Voigt model, which were used previously to model larval musculature (10,39), could

not fit the experimental curve well since either exponential decay or residual elastic force was

missing in these models (Supplementary Figure 2). In contrast, the standard linear solid

(SLS) model, which combined the Maxwell model and a Hookean spring in parallel (52)

(Figure 4I), fitted the experimental results well. Thus, we fitted this curve with the general

SLS model (Figure 4H left). According to the SLS model, we obtained the two spring

constants and one damping coefficient for the whole body of intact larvae by the extension

of 0.4 mm (k_1^{whole} = 3.7 ± 0.7 mN/mm, k_2^{whole} = 5.3 ± 1.1 mN/mm, c^{whole} = (2.4 ± 0.5) × 10^2

mN sec/mm, from n = 6 larvae, Figure 4J-4L). Consistent values were obtained by the

extension of 0.6 mm (k_1^{whole} = 2.5 ± 0.4 mN/mm, k_2^{whole} = 6.1 ± 1.1 mN/mm, c^{whole} = (2.6 ±

0.2) × 10^2 mN sec/mm, from n=5 larvae, Figure 4J-4L), which further supported the linear

property of larvae. The two spring constants didn't have a strong correlation (r = 0.49, p =

0.13, n = 11; Pearson's Correlation Coefficient) suggesting that they could not be reduced to

a single spring constant. To sum, we obtained the viscoelastic parameters of larvae, two

spring constants and one damping coefficient, by the stress relaxation test. It should be noted

that in larval crawling, each segment exhibited contraction instead of extension which we

induced in the measurement. However, we could not measure the viscoelasticity of larvae

during contraction since larvae were bent instead of compressed when pushed from both

ends. Accordingly, we assumed larvae possess the same linear viscoelastic properties both

in extension and compression. It should also be noted that in larval crawling each segment

contracts by about 0.2 mm (Figure 2B) while in the stress-relaxation experiment each

segment was extended by about 0.04 mm (0.4 mm / 11 segments). There could be some

non-linearity in the viscoelastic properties of the larval body. However, in our model we

adapted the viscoelasticity measured with 0.4 mm extension as the approximate values for

our mathematical model of larval crawling.

A neuromechanical model for larval crawling referring to the physical measurement

We established a mathematical neuromechanical model based on the physical

measurements described above. We obtained seven kinematic values characterizing

crawling locomotion (Figure 5A) from the measurement of fly larvae (Figure 1 and 2). Our

aim was to build a model with a neural circuit and mechanical components to reproduce the

observed results quantitatively. Regarding the mechanical part, based on the measurements,

we estimated that the larva was a chain of eleven consistent segments (Figure 2), each of

which was described by the SLS model (Figure 4 and Supplementary Figure 1). These

assumptions indicated that the viscoelastic parameters for single segments in the model (two

spring constants k_1 and k_2 and one damping coefficient c) should be 11 times larger than the

ones for the whole body (k_1 = 40.7 mN/mm, k_2 = 58.3 mN/mm, and c = 2640 mN sec/mm).

Furthermore, the force measurement indicated that the maximum muscular contraction force

could be 6.7 mN (Figure 3). We modelled segmental boundaries as masses that were pulled

and pushed by segmental muscles and dragged on the surface with friction (Figure 5B). We

measured the mass of larvae (1.14 mg, the 99% confidence interval is [1.12, 1.15], n = 70

larvae) and calculated the mass of one segment by dividing the mass of the whole body by

the number of segments to obtain 0.1 mg/segment. The length of larvae was 3.5 ± 0.1 mm

(n = 9). We used all these values in our mechanical model (green parameters in Figure 5B).

In contrast, as for the neural network part, we adapted a neural circuit model built by

Pehlevan *et al.* (2016) based on Wilson-Cowan equations. This model was capable of

generating propagation of waves from the posterior to anterior segments by interaction

among excitatory and inhibitory neurons in the central nervous system (CNS), motor neurons,

and sensory neurons (10). Although the parameters in this model were suggested, we

incorporated the neural circuit framework and tuned its parameters to build a

neuromechanical model based on physical measurement to reproduce larval crawling.

Aiming to reproduce the measurement results on larval crawling, we adjusted 15

parameters in the neural circuit model (magenta parameters in Figure 5B). The optimized set

of the parameters (Supplementary Figure 3) could reproduce the measurement results of the

kinematics (Figure 5C-5F). To assess this observation quantitatively, we compared the seven

kinematics parameters (Figure 5A) between the measurement and simulation and found that

all the parameters could be reproduced by the simulation to fit in the ranges of the

measurement results (Figure 5G-5M). Accordingly, this neuromechanical model could

quantitatively describe the segmental kinematics during forward larvae crawling.

The stress-relaxation results showed large variabilities on the order of 100% of the

mean values (Figure 4J-4L). This variance could be caused by the uncertainty in the

measurement or the variability in physical properties among larvae. Since we didn't have

independent measurement methods to obtain viscoelasticity, we couldn't determine which

one was the case. However, when we perturbed the spring constants by the order of 100%

of the optimized value, crawling speed changed to be out of the measured range

(Supplementary Figure 4). This observation suggested that the viscoelasticity would be

consistent between larvae, and the variabilities in the stress-relaxation test would be caused

by uncertainty in the measurement.

We adapted μ_{bf}, the asymmetricity parameter between forward and backward

friction as 10 considering the fact that a larva had denticle belts on the ventral side of the

body, providing asymmetric friction with the ground. To test the dependency of crawling on

this asymmetricity, we perturbed μ_{bf} (Supplementary Figure 5). The simulation results

showed that crawling speed didn't change even when μ_{bf} equalled one, meaning that the

friction was symmetric between forward and backward. This observation indicated that the

asymmetricity in the friction along the body axis had a small role in generating forward

crawling.

As for the maximum muscular contraction force, we adapted the maximum force

observed by optogenetic stimulation. To test whether we could use smaller muscular forces

to reproduce larval crawling, we conducted a perturbation analysis on the maximum muscular

force in our neuromechanical model (Supplementary Figure 6). The simulation results

showed that crawling speed reduced as the muscular force decreased. Accordingly, this

observation suggested that crawling speed was sensitive to the maximum muscular force

and the measurement of contraction force was crucial to build a neuromechanical model for

larval crawling.

We compared parameters in our model based on physical measurements with those

in the previous simulation by Pehlevan *et al.* (2016). In Pehlevan *et al.* (2016), parameters

were scaled by three values, the spring constant k, the equilibrium length of one segment L,

and the relaxation time scale of the excitatory neurons τ_E. Accordingly, we substituted these

parameters with our measurement results (k = 50 mN/mm, L = 0.35 mm, and τ_E = 35 msec)

and obtained the absolute values of the parameters. By comparison, we found that the neural

couplings and relaxation times in the CNS were almost consistent between our results and

the assumption in Pehlevan *et al.* (2016). On the other hands, physical properties showed

clear contrast between them. The damping coefficient in our result ($c \sim$ 2640 mN sec/mm)

was about 400 times larger than the previous assumption (10) ($c \sim$ 6 mN sec/mm). When we

adapted the damping coefficient 400 times smaller than our value, crawling speed was

affected to be doubled (crawling speed: 0.69 mm/sec in the optimized condition; 1.32 mm/sec

when the damping coefficient c was 400 times smaller than the optimized value of c,

Supplementary Figure 4C). And the maximum muscle contraction force in our results (F_{Mmax}

= 6.7 mN) was 2.2 times smaller than the previous assumption (10) (F_{Mmax} = 15 mN). In

addition, neural couplings between the CNS and either muscles or sensory neurons also

exhibited differences: The coupling between the excitatory neurons and muscles in our model

(w_{tE} = 540) was larger the previous assumption (w_{tE} = 1 in (10)), and the couplings between

the sensory neurons and the CNS in our model ($w_{ES} = w_{IS}$ = 300) were also larger than the

previous assumption ($w_{ES} = w_{IS} = 1.95$ in (10)). To sum, our mechanical model had larger

viscosity and smaller muscular force whereas the circuit model had larger couplings between

the CNS and their targets in the peripheral structures than the assumption in the previous

theoretical work.

The model reproduces previous observations in optogenetic experiments

To validate our model, we simulated two optogenetic perturbation studies reported

previously and compared the results with the experimental observations (32,53). First, by

optogenetic silencing of motor neurons in a few segments, propagation of contraction from

the posterior to anterior segments was arrested, and all the segments were relaxed (53). In

the previous simulation study (10), although propagation was arrested by silencing the

excitatory group in one segment, its neighbouring segment kept contracted instead of being

relaxed. We silenced excitatory neurons in the A3 segment for 2 seconds in our

neuromechanical model (Figure 6A-6F) and found that the silencing arrested the propagating

wave (Figure 6E). Furthermore, all the segments were relaxed by this optogenetic silencing

(Figure 6F), which is consistent with the experimental observation (53). Inada *et al.* (2011)

demonstrated that crawling was resumed after removing optogenetic silencing (53). This

phenomenon was not reproduced in our simulation: No wave was generated after

optogenetic silencing (Figure 6E and 6F), although waves were resumed after a short period

of silencing (Supplementary Figure 7). As pointed out in Pehlevan *et al.* (2016), this would

be due to the lack of such a mechanism in the neural circuit model. To sum, our model

successfully reproduced the observation that the silencing excitatory neurons, particularly

motor neurons, in a single segment arrested the propagation of peristaltic waves and relaxed

all the segments.

Next, we tested the effect of activation of inhibitory neurons on crawling behaviour.

A previous study reported that activation of inhibitory premotor interneurons PMSIs arrested

wave propagation and caused the relaxation of the whole body (32). Therefore, we activated

inhibitory neurons in the A3 segment in the neuromechanical model (Figure 6G). By this

treatment, waves were arrested (Figure 6H), and the whole segments returned back to their

equilibrium length (Figure 6I). Accordingly, our neuromechanical model successfully

reproduced the two optogenetics experiment results.

347   Measurement of forward crawling behaviour in a low-friction condition and validation

348   of the model

Friction was a reaction force of a propelling force that drove larval movement.

Although friction was necessary to move the centroid of larvae, it was unclear whether friction

was required to generate the patterned segmental motion. In the previous theoretical study,

two phenomena in segmental dynamics in a low friction condition were simulated: Each

segment contracted more, and intersegmental propagation delay became longer (10). Our

neuromechanical model tested the segmental dynamics in no friction condition (Figure 7A-

7H). The simulation results showed that the range of segment contraction didn't change even

in the no friction condition (Figure 7C – 7F). Also, the duration of segmental contraction was

not affected either (Figure 7G). Furthermore, with respect to the wave propagation,

intersegmental delay was not changed in no friction condition (Figure 7H). Accordingly, in

our mathematical model, segmental dynamics was robust in the no friction condition.

To reveal the roles of friction on larval crawling, we measured body segment

kinematics in crawling larvae in a low-friction environment. We used a high concentration

sugar solution (66% w/w sucrose) and floated third-instar larvae on it. To visualize segment

boundaries of larvae, we used *tubP-Gal4, UAS-fondue::GFP* fly larvae as described above

(Figure 1A). We compared the crawling motion between on the agarose substrate (Figure 7I)

and in the sugar solution (low friction environment) (Figure 7J). Floating larvae could exhibit

crawling behaviour (Figure 7I), suggesting that the interaction with a substrate was not

required to generate peristaltic motion. They could not move forward in the sugar solution

probably due to lack of the propelling force that was the reaction force of friction or because

of viscous resistance in the sugar solution. The number of waves was fewer in floating larvae

than larvae on an agarose substrate (agarose: 45.5 ± 3.5 crawls/min, n = 6 larvae; floating:

6.8 ± 2.6 crawls/min, n = 6 larvae; p = 9.0×10^{-6}, Welch's t-test; Supplementary Figure 8A).

This observation implied that friction could be involved in the initiation of crawling. This

phenomenon could not be observed in our neuromechanical model (Supplementary Figure

8B) probably because our model didn't include a mechanism to control the initiation of waves

independent of the completion of waves. How each crawling wave was initiated and how the

temporal gap between consecutive waves was regulated remained important open questions.

Since our focus in this study was on the segmental and intersegmental dynamics, we

analyzed the kinematics of every single peristaltic wave.

First, we examined the segmental dynamics in the low friction condition and found

that the range of segment contraction didn't change in most of the segments in floating larvae

(Figure 7K and 7L). In addition, the contraction duration of each segment was not affected in

the floating condition (Figure 7M). These observations were consistent with our model results

(Figure 7E-7G). In the posterior segment A6 and A7, however, there was a difference

between larvae on agarose and floating larvae. The range of contraction at the posterior

segments was reduced in floating larvae (Figure 7L). Since forward crawling started at the

posterior segments, this observation implied that friction would be crucial to initiate crawling.

This implication was consistent with the observation of the reduction in crawling numbers in

floating larvae (Supplementary Figure 8A). Second, we analyzed the intersegmental delay in

the floating larvae. In most segments, intersegmental delay was consistent between larvae

on agarose and floating larvae (Figure 7N). However, the intersegmental delay between T3

and A1 was increased in floating larvae. Since this phenomenon was observed in the limited

anterior segment, it would be possible that other behaviour, including head-sweeping that

occurs in the anterior segments, was affected in the low friction condition. To sum, the

kinematics in larval crawling was almost similar between on the agarose substrate and in

low-friction condition. This observation was consistent with the result of our neuromechanical

model.

Contribution of sensory feedback and CNS

The CNS and proprioception were both involved in locomotion. The significant

contribution of sensory feedback in larval crawling was shown experimentally (Hughes and

Thomas 2007). This observation raised a hypothesis that proprioception could cause the

propagation signal to the neighbouring segment through intersegmental sensory feedback

(44). A simulation based on this assumption showed that the model circuit with

intersegmental feedback could normally generate propagation waves without an

intersegmental connection in the CNS (10). On the other hand, several key interneurons

regulating larval locomotion had been identified (32,54–56), suggesting that interneurons in

the CNS should be involved in wave propagation. Aiming to reproduce the experimental

observation of the involvement of the CNS in crawling, we tested the contribution of

intersegmental sensory feedback and the intersegmental connection in the CNS to peristaltic

motion by our neuromechanical model (Figure 8). When the sensory feedback was silenced

($w_{ES} = 0$), crawling speed was reduced (Figure 8B, 8D, and 8H). This was consistent with

previous simulation result (10) and the experimental result (44). When the intersegmental

central connection was blocked ($w_{En} = 0$), the speed of crawling was decreased too (Figure

8B, 8F, and 8I). This result was also consistent with observations that interneurons in the

CNS were involved in crawling speed. While the speed was reduced in both cases, the neural

mechanisms would be different. When sensory feedback was blocked, the activity of

inhibitory neurons was attenuated (Figure 8C and 8E). Meanwhile, when the intersegmental

central connection was blocked, the activity of inhibitory neurons was enhanced (Figure 8C

and 8G). This observation suggested that sensory feedback and the CNS were involved in

the speed control by distinct mechanisms. To examine their roles in detail, we perturbed w_{ES}

and w_{En} from the optimal values. The speed of crawling was robust to the change of w_{ES}

(Figure 8H), whereas increase in w_{En} led to drastic change in crawling speed (Figure 8I). In

particular, crawling speed depended on w_{En} nonlinearly with a peak. To sum, this simulation

result was consistent with the experimental observations that interneurons in the CNS should

be involved in the regulation of crawling behaviour.

426   Next, we analyzed the interaction between intersegmental sensory feedback and

intersegmental connection in the CNS. We perturbed w_{En} and w_{ES} simultaneously and

plotted the displacement of larvae in a two-dimensional plot (Figure 9A). The plot showed

that crawling could be realized in the wide area of this parameter space. When w_{En} was

larger than the value in the optimized condition (0.6), w_{En} played a dominant role in speed

control compared to w_{ES} (Figure 9B). On the other hand, in the regime of smaller w_{En}, both

w_{En} and w_{ES} were involved in crawling speed. This result indicated the strength of central

connectivity in the CNS should play a pivotal role to control the speed of crawling behaviour.

Contribution of excitatory and inhibitory neurons in crawling

436   Based on the observation suggesting a significant contribution of the CNS to crawling

behaviour, we next examined the involvement of excitatory and inhibitory neurons in larval

locomotion. To this aim, we perturbed intrasegmental connection weight: w_{EE} for excitatory

connections and w_{EI} for inhibitory connections (Figure 10A-10G). Crawl speed decreased

when blocked excitatory connections (Figures 10B and 10D). Since the traces of excitatory

and inhibitory neurons were different from those in blocking intersegmental excitatory

connections (Figure 8E and 10E), the speed reduction mechanism should be different

between silencing the intrasegmental excitatory connections and intersegmental excitatory

connections. On the other hand, when the activity of inhibitory neurons was suppressed,

larvae couldn't exhibit crawling (Figure 10F). In this case, all the neurons exhibited tonic

hyperactivity due to a lack of inhibition (Figure 10G). To further reveal the involvement of w_{EE}

and w_{EI}, we perturbed them in the range where larvae could exhibit crawling. The plots

showed that speed was related to w_{EE} and w_{EI} in non-monotonical manners (Figure 10H and

10I). This observation indicated that both excitatory and inhibitory neurons controlled

crawling speed.

Next, we analyzed the interaction between excitatory and inhibitory neurons.

Displacement of larvae with different values of w_{EE} and w_{EI} was plotted two-dimensionally.

The diagram indicated that when w_{EE} was large and w_{EI} was close to zero (the upper right

side of the diagram), larvae couldn't generate crawling (Figure 11A). On the other hand, when

w_{EE} was small (weak excitatory connection) or w_{EI} was small (strong inhibitory connection)

that corresponded to the lower-left region of the diagram, crawling speed was reduced.

Interestingly, as long as w_{EE} and w_{EI} were balanced (the diagonal region of the diagram),

crawling speed was consistent. The deviation in speed when w_{EE} and w_{EI} were perturbed

was within the range of variability observed experimentally (Figure 11B). These results

indicated two points: The balance between excitatory and inhibitory connections within

segments was critical to generate peristaltic motion. And, as long as they were balanced,

crawling speed would not change by perturbation in intrasegmental connection weights.

Prediction in the neural network in sister species of *Drosophila melanogaster*

Comparison between the contribution of intersegmental (Figure 9B) and

intrasegmental (Figure 11B) connections to crawling speed suggested that intersegmental

connections in the CNS had dominant roles in regulating crawling speed. We noticed that

this observation could allow us to predict neural circuits for fly larval crawling. A recent study

reported an inter-specific variation in crawling speed among eleven species in the genus

Drosophila (57). This study showed that some sister species crawled faster than *Drosophila*

melanogaster, and the others locomoted slower. We attempted to make a prediction about

the intersegmental connection in the CNS of these species based on their crawling speed.

To predict the property of neural circuits in these sister species, we overlaid the speed data

of the species on the graph showing speed dependency on w_{En} (Figure 12). To compensate

the difference in experimental conditions between this study and Matsuo *et al.* (2021), the

speed of each species was normalized based on the speed of *Drosophila melanogaster*. To

show the dependency on w_{En}, the dependency of w_{ES} was averaged out from Figure 9B. As

a result, all of the eleven horizontal lines demonstrating the crawling speed of sister species

crossed to the speed-w_{En} relation curve (Figure 12). This plot suggested that some species

showing faster crawling, *Drosophila pseudoobscura* for example, should have strong

intersegmental connections in the CNS while those crawling slower such as *Drosophila*

mojavensis, should have weaker intersegmental central connections. This prediction would

be testable by interspecific comparison based on the anatomy of their central nervous system

or physiological recording.

Discussion

In this work, we built a neuromechanical model based on the physical properties of

fly larvae. The model successfully described crawling behaviour quantitatively. First, we

quantified segmental dynamics in larval crawling and obtained seven parameters that

characterize the kinematics of peristalsis (Figures 1 and 2). Then, using a tensile tester,

viscoelasticity and tension force of larvae were measured (Figures 3 and 4). These results

suggest that the larval body could be modelled as a chain of mass and SLS modules (Figure

4), distinct from the previous modelling for larvae (10,39,41). By incorporating the material

properties and optimizing parameters in the neural circuit, our model succeeded in

reproducing larval crawling quantitatively (Figure 5). Furthermore, this model could describe

the observation in optogenetic studies (Figure 6) and crawling in a low friction condition

tested in this study (Figure 7). Perturbation analyses indicated the importance of

intersegmental connections in the CNS, contrasting to previous studies (Figures 8 and 9).

Based on this observation, we predicted the intersegmental connections in the CNS in sister

species in the genus *Drosophila* (Figure 12).

One striking finding from our model contrasts with previous studies: the significant

contribution of intersegmental connections in the CNS to crawling speed. Although several

interneurons involved in speed control have been reported (32,54–56), previous simulation

studies were not consistent with these observations. Our model had larger viscosity and

smaller contraction forces (Supplementary Figure 3) than previous parameter regimes,

implying that each segment is hard to move. The large weight of neuromuscular connection

compensated for this difficulty (w_{ME}) and that of sensory feedback (w_{ES}) (Supplementary

Figure 3). With the strong interaction between the CNS and peripheral organs (muscles and

proprioceptors), the CNS could play a significant role in controlling crawling speed (Figure

8I). This finding demonstrates the significance of intersegmental connection in the CNS. It

also highlights the importance of mechanical properties in the larval body and the dynamics

of segments.

We measured the viscoelastic properties of larvae by the stress-relaxation test. It

should be noted that there are some limitations in this measurement. First, we obtained these

passive properties of the body by measuring unanaesthetised larvae. We analyzed the data

without any spontaneous contraction in the stress-relaxation test. However, there remains a

possibility that infinitesimal muscular tension is induced by proprioceptive feedback upon

stretching. By blocking action potentials in motor neurons while keeping spontaneous vesicle

release, it would be able to suppress feedback from proprioception to measure purer

viscoelasticity. Second, we approximated the viscoelasticity for the contraction in the range

of 0.2 mm by that for the extension in the range of 0.04 mm. In real larval crawling,

asymmetricity between extension and contraction and nonlinearity in the viscosity would

affect the kinematics. By incorporating these factors, it would be able to reproduce the

kinematics more quantitatively.

The model in this study could describe forward crawling, the most frequent behaviour

in larvae. Recent neuroscience studies have revealed numerous neural circuit modules

involved in distinct aspects of behaviour, including speed control (32), bilateral coordination

(35), intrasegmental coordination (36), intersegmental coordination (31), backward crawling

(58,59), turning (60), escaping (61), and sensory input guided navigation (34,62). By

integrating these circuit modules, we would be able to establish a neuromechanical model

that reproduces multiple and natural larval behaviour. Furthermore, our model can potentially

serve biomimetics. In recent decades, more and more soft robots, endowed with new

capabilities relative to the traditional hard ones, have been designed to exhibit complex

movements (63–66). Taking *Drosophila* larvae as a prototype, bionic structures can be

established with high dexterity to explore the unstructured environments. By harnessing

perturbation analyses on the neuromechanical model, the locomotion ability of the soft larval

robots could be tuned and optimized for required applications.

Materials and Methods

Fly strains

We used the third instar larvae in all the experiments. To quantify segment dynamics,

we used *tubP-Gal4*, *UAS-fondue::GFP* (Bloomington #5138, #43646), which labels the

segment boundaries (45). In the viscoelasticity measurements, we used a wild type strain

Canton S. For optogenetic experiments, *OK6-Gal4* (67) and *UAS-ChR2[T159C]::YFP* (31)

were used.

Image acquisition and segment boundary annotation

Third instar larvae of *tubP-Gal4, UAS-fondue::GFP* were gently washed in deionised

water to remove residual food from the body surface. Then, individual larvae were placed on

a flat agarose stage (1.5% agarose). Behavioural videos were captured by a CCD camera

(XCD60, Sony, Japan) mounted on an Olympus stereomicroscope (SZX16, Olympus, Japan).

Images were acquired at 30 Hz. We used Fiji software (68) to manually annotate the right

and left ends of every segment boundary (from the anterior boundary of the T2 segment to

the posterior boundary of the A8 segment. See Figure 1A.) The midpoint of the right and left

ends of a boundary was used as the position of the boundary.

Viscoelasticity measurement

Third instar larvae in the feeding stage were washed with distilled water and dried

with paper. Insect pins were inserted into the head and tail. The pin in the head was bent to

form a loop to hook to a paper clip that was hung on the hook of the tensile sensing machine,

while the pin in the tail was used to fix the body on the PDMS (Polydimethylsiloxane, Sylgard

184, Toray, Japan) silicone block, held by the tong on the SHIMADZU EZ-S platform with a

5 N load cell. The experimental equipment is shown in Figure 4A. The larval body was kept

on the vertical axis for measurement. The baseline of force was calibrated by values

measured before applying external elongational force. All the experimental procedures were

performed at room temperature.

During the stress relaxation tests, we applied a constant strain of 0.4 mm, about 10%

of the body length (3.53 ± 0.12 mm, n = 9 larvae), to the larvae. Then, the stress decreased

until the plateau was reached after a while, as shown in Figure 4G-4H. To fit the stress

relaxation curve to mechanical analogues, we adapted the Maxwell, Kelvin-Voigt, and

standard linear solid (SLS) models. These models give the relationship between joint force

F and displacement ΔL. Detailed functions are described as follows:

$\quad \frac{F}{c} + \frac{1}{k}\frac{dF}{dt} = \frac{d\Delta L}{dt}$ Maxwell model

$\quad F = k\Delta L + c\frac{d\Delta L}{dt}$ Kelvin-Voigt model

$\quad F + \frac{c}{k_2}\frac{dF}{dt} = k_1\left(\Delta L + c\frac{k_1+k_2}{k_1 k_2}\frac{d\Delta L}{dt}\right)$ SLS model

where k and c are the elastic and damping constants, respectively. The total displacement

of 0.4 mm was realised by pulling the larval body with a rate of 1 mm/min. During the stress

relaxation experiments, this elongation time (24 sec) is much shorter than that for relaxation

(576 sec), and thus the displacement is regarded as the step function $L(t) = L_0 H(t - t_0)$ and

initial force is $F(0) = 0N$, where $L_0 = 0.4\ mm$ and $H(t)$ is the Heaviside step function. In this

case, the corresponding stress relaxation functions in these models are described as follows:

$\quad F = ke^{-\frac{k}{c}(t-t_0)}L_0 H(t - t_0)$ Maxwell model

$F = kL_0H(t - t_0) + cL_0\delta(t - t_0)$ Kelvin-Voigt model

$F(t) = \left[k_1 + k_2e^{-\frac{k_2(t-t_0)}{c}}\right]L_0H(t - t_0)$ SLS model

where $t_0 \geq 0$. By fitting these curves to the stress-relaxation measurement data, we obtained

the spring constants and damping coefficients. We used Python 3.7 for the curve fitting.

Contraction force measurement with optogenetics

For optogenetic activation of motor neurons, we used the *OK6-GAL4, UAS-ChR2*

line (32). The early third-instar larvae were selected and put into ATR (all-trans-retinal)

containing yeast paste, the concentration of which was 1 mM. These larvae were reared at

25 °C in the dark for one day (69). Afterwards, the third-instar larvae were prepared to

measure tension force as described above (Viscoelasticity measurement section). Blue LED

light (455 nm, 5.7 nW/mm^2, M455L3, ThorLab) was used to stimulate ChR2 expressed in

motor neurons, which leads to the contraction of the larval body. In each stimulation, the blue

light was applied for two seconds followed by a no-illumination interval of two seconds, and

the force induced was monitored. Eighteen larvae were used in the measurement, and each

measurement took two to five minutes. The optogenetically induced forces were measured

by the differences between forces during illumination and no illumination (Figure 3).

Larval crawling in a low-friction environment

We used a high concentration sugar solution (66% w/w sucrose) and floated third-

instar larvae in it. The genotype we used was *R70C01-Gal4, UAS-CD4::GFP*, which allowed

us to mark the segmental boundary from T2 to A8 (Figure 1A and 1B). The locomotion was

recorded via SZX16 fluorescent microscope (Olympus, Japan) with a 1.25x object lens at 30

frames/sec, and its trajectory was measured by Fiji (68).

Modelling

Body-substrate mechanics and modelling

As we mentioned before, the larval crawling stride consists of a piston phase and a

wave phase (26). The piston phase constrains the larval body length to be almost constant,

while the wave phase generates the propagation wave repetitively. To make it simple, we

modelled the whole body of larvae as a chain of eleven segments.

We assumed that the model framework possesses a constant length and its

segments are entirely repetitive based on the observation in Figures 1 and 2. Then the body

is modelled as a chain of the SLS units in series (Supplementary Figure 1). Muscle groups

are modelled as the tension actuator to accept efferent control from the neural circuit (Figure

5B). The tension F_M is the contraction force to counteract the effect of body viscoelasticity

and friction. The mechanics are described based on Newton's second law as follows.

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$$\begin{cases} m\ddot{y}_{-1} = m\ddot{y}_{10} = F_{10} - F_0 + F_{M_{10}} - F_{M_0} - f_{-1} \\ m\ddot{y}_i = F_i - F_{i+1} + F_{M_i} - F_{M_{i+1}} - f_i \quad i = 0, \dots, n-2 \\ y_{-1} = y_{10} + nL \end{cases}$$

$$F_i + \frac{c}{k_2}\frac{dF_i}{dt} = k_1\left(y_{i-1} - y_i - L + c\frac{k_1+k_2}{k_1 k_2}\left(\frac{dy_{i-1}}{dt} - \frac{dy_i}{dt}\right)\right)$$

$$\tau_M \dot{F}_{M_i} = -F_{M_i} + F_{M_{max}} \sigma_M(w_{ME}E_i - \theta_M) \quad i = 0, \dots, n$$

$$\sigma_M(v) = \frac{1}{1+e^{-k_M v}}$$

where y_i is the segmental boundary position (Figure 1B and Supplementary Figure 1), m is

mass, F is viscoelastic force, F_M is tension force, τ_M is time relaxation constant for tension,

w_{ME} is connection weight from excitatory unit to tension actuator, θ_M is the threshold for

tension, and k_M is the gain in function $\sigma_M(v)$, and n is the total number of segments, equal

to 11. y_{-1} is the position of the head and y_{10} is the position of the tail. To model the piston

phase, where the head and tail move concurrently, the posterior and anterior ends share the

same velocity during crawling, as $\dot{y}_{-1} = \dot{y}_{10}$ which is inferred from the third equation above.

Each mass block is dependent on joint force from SLS modules, tensions, and friction. The

joint force from the SLS unit is affected by the segmental displacement, and the tension force

is regulated by the sigmoid function with gain k_t. The periodic tension force, modelled by the

sigmoid function of excitatory inputs with gain k_M, is indispensable to sustain the propagation

of contraction wave, verified by the experimental results (53).

As for the friction force, it exists during the interaction of the mechanical body with

the substrate. The transition process from static to dynamic friction is not modelled in this

work. Instead, the ratio of forward to backward friction is introduced to the model as

directional asymmetric, considering the anterior-posterior polarity in denticle bands. Since

the backward friction is larger than forward friction, the ratio is more than one. Friction on the

segmental boundary is represented as:

$$f_i = \begin{cases} F_{i,ext} & \dot{y}_i = 0 \ and \ -\mu_{bf}F_f \le F_{i,ext} \le F_f \\ F_f(\sigma_f(\dot{y}_i) - \mu_{bf}\sigma_f(-\dot{y}_i)) & otherwise \end{cases} \quad i = -1, 0, \dots, n-1$$

$$\sigma_f(v) = \frac{1}{1+e^{-k_f v}}$$

where f, F_f, μ_{bf} ($\mu_{bf} > 1$) individually represent the friction, forward friction and ratio for

forward-backward friction, and $F_{i,ext}$ refers to the joint force of all the other forces. When the

mass block is still and $F_{i,ext}$ does not exceed the range of forward-backward friction, the

friction force f_i should be equal to $F_{i,ext}$. Otherwise, the friction is either the forward friction

F_f or the backward one $\mu_{bf}F_f$.

Neuromuscular dynamics and modelling

The framework for the neural circuit is depicted in Figure 5B. The neural circuit model

is based on the model in Phelevan *et al*. (2016). Neural dynamics is realized by the activities

of excitatory and inhibitory populations of neurons in each segment under the Wilson-Cowan

model (70,71). In *Drosophila* larvae, most proprioceptive neurons were active when the

segment was contracted (43). The feedback from the sensory receptor provides signals for

the inhibitory neuron within the same segment and excitatory neuron in the anterior segment.

In this case, it can promote both local relaxation and forward propagation waves. This

connectivity is consistent with the "mission-accomplished" model (44).

Under these assumptions, neural dynamics of neural circuits are depicted as follows:

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$$\begin{cases} \tau_E \dot{E}_i = -E_i + \sigma_E(w_{EI}I_i + w_{EE}E_i + w_{En}E_{i+1} + w_{ES}S_{i+1} - \theta_E) & i = 0, \dots, n-2 \\ \tau_I \dot{I}_i = -I_i + \sigma_I(w_{IE}E_i + w_{IS}S_i - \theta_I) & i = 0, \dots, n-2 \\ \tau_E \dot{E}_{10} = -E_n + \sigma_E(w_{EI}I_{10} + w_{EE}E_{10} + w_{En}E_0 + w_{ES}S_0 + ini - \theta_E) \\ \tau_I \dot{I}_{10} = -I_{10} + \sigma_I(w_{IE}E_{10} + w_{IS}S_{10} - \theta_I) \end{cases}$$

$S_i = \sigma_S(L\theta_S - y_{i-1} + y_i)$ $i = 0, \dots, n-1$

$\sigma_E(v) = \frac{1}{1+e^{-k_E v}},\qquad \sigma_I(v) = \frac{1}{1+e^{-k_I v}},\qquad \sigma_S(v) = \frac{1}{1+e^{-k_S v}}$

where E and I are the mean firing rates of the excitatory and inhibitory population, τ_E and τ_I

are the relaxation time constant of the excitatory and inhibitory units, respectively, w_{ab} is their

synaptic connection weight from population b to population a, θ_E and θ_I are the activation

threshold of the excitatory and inhibitory units, k_E, k_I, and k_S are the sigmoid gain of

excitatory, inhibitory, and sensory units, respectively, and S is the feedback strength from the

sensory receptor. The circuit includes excitatory connection via w_{IE}, w_{ME} and inhibitory

connection via w_{ES}, w_{EI}. When the segmental length becomes smaller than the threshold $L\theta_S$,

the sensory unit starts to be activated. To trigger the initial crawling, we introduced an

external stimulus ini, a rectangular pulse (for 5 ms), on the excitatory population in the

posterior terminal.

The values of the parameters are listed in Supplementary Figure 3. All the simulation

work is performed using stiff solver ode15s in MATLAB R2020a.

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Competing interests

We have no conflict of interest with respect to the work.

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Figure 1. Characterization of forward crawling in third-instar larvae. (A) A fluorescence

image of a third-instar larva with the anterior to the top. The segmental boundaries were

visualized using *tubP-Gal4, UAS-fondue::GFP*. (B) A schematic of the segment boundaries

(y0-y10) and the segment names (T2-A8). (C) Displacement of the segment boundaries

during larval crawling. (D) Kinematics parameters based on segmental boundary dynamics.

(E) A schematic of the segment names. (F) Segment length changes during larval crawling.

(G) Kinematics parameters in segmental length change.

Figure 2. Consistent kinematics properties among segments in larval crawling

(A) A schematic of the segment names. (B) The range of segment length changes during

larval crawling. Upward and downward triangles show the maximum and minimum length of

the segments, respectively. (C) Contraction duration in larval segmental dynamics. (D)

Displacement speed of larval segmental boundaries and schematics of their intersegmental

delay. (E) Linear regression for larval intersegmental delays. (F) Effective segment numbers

estimated by linear regression in (E).

Figure 3. Measurement of contraction force in larvae

(A) A larva was hooked at the head and tail. The extension and tensile force of the larva were

measured by a tensile tester. (B) A sample trace of spontaneous contraction force of a larva.

(C) Optogenetic stimulation to a larva during measurement with the tensile tester. (D) A

sample trace of larval force with optogenetic activation (shown in blue bars above the trace).

(E) The tensile force of larvae generated by spontaneous contraction ("Spt"; n=11 contraction

events from three larvae) and optogenetic activation ("Opt"; n=44 activations from seven

larvae).

Figure 4. Measurement of viscoelasticity of the larval body

(A) Measurement and control of extension and tensile force of larval body with the tensile

tester. The double-headed arrow indicates that the extension is changeable during the

measurement. (B) A schematic of tensile force and extension of a larva. The left larva is not

subjected to external forces while the right one is extended. The applied force to extend is

the tensile force. (C) In the measurement of the relationship between extension and tensile

force, the larvae were extended at a constant rate as shown in this panel, and the tensile

force is being recorded. (D) An example trace of the relationship between extension and

tensile force. (E) Plots of (D) in two different ranges of extension (Left: 0-0.4 mm, right: 0-1.0

mm). Green lines indicate linear regression lines in these ranges. (F) The coefficient of

determination of linear regression in different ranges of extension. (G) In the stress-relaxation

test, the larvae were extended quickly, and their length was kept constant. The tensile force

under the constant extension was being recorded. (H) Example traces of stress-relaxation

tests with the constant strain of 0.4 mm (left) and 0.6 mm (right). Fitting curves with the SLS

model are shown in green (left) and magenta (right). (I) By the SLS model, the whole larval

body can be described as two springs (spring constants: k_1^{whole} and k_2^{whole}) and one damper

(damping coefficient: c^{whole})   (J-L) Scatter plots of k_1^{whole} (J), k_2^{whole} (K), and c^{whole} (L)

measured with the maximum strain of 0.4 mm (green) and 0.6 mm (magenta).

Figure 5. Reproduction of larval crawling by a neuromechanical model

(A) Kinematics parameters in segmental boundary dynamics (left, same as Figure 1D) and segmental length change (right, same as Figure 1G). (B) A schematic of our neuromechanical model for larval crawling. The neural circuit was referred to Pehlevan *et al.* (2016), although the parameter values in the model were different. Two segments in a larva

(corresponding to the dotted box below) are drawn. Circles are populations of neurons: E_i is

an excitatory neuron group, I_i is an inhibitory neuron group, and S_i is a sensory neuron group

in the i-th segment. Excitatory and inhibitory connections are labelled by red and blue arrows,

respectively. The body of the i-th segment is modelled by two springs (k_1 and k_2), one

damper (c), and one muscle whose force is M_i. Segment boundaries have masses (m) that

feel friction with the substrate (F_f in forward motion and $\mu_{bf}F_f$ in backward motion). The

position of the i-th segment is denoted as y_i. (C) A kymograph of segmental boundaries

during larval crawling (same as Figure 1C). (D) Change in segmental length during larval

crawling (same data shown in Figure 1G). (E) A simulation result of kymograph of segmental

boundaries. (F) Simulation result of segmental length. Segment labels and line colours in (C)

and (E) correspond to those in Figure 1B and 1C. (G-L) Comparison of seven kinematics

between parameters obtained from larval crawling (black dots, n = 9 larvae) and simulation

(red dots). (G) Stride length. (H) Stride duration. (I) Intersegmental delay. (J) Crawling speed.

(K) Maximum segment length. (L) Minimum segment length. (M) Contraction duration of

single segments.

Figure 6. Reproduction of optogenetic experiments by the mathematical model.

(A) A schematic of two segments in the mathematical models. (B) Activity of excitatory (solid

lines) and inhibitory neurons (dotted lines) in A8-T2 segments by the model without

optogenetic perturbation. (C) Traces of segment length in (B). Dotted lines denote the

equilibrium length of the segments. A time period of 3.5-4.5 seconds is shaded to compare

with (F) and (I). (D) A schematic of optogenetic silencing of excitatory neurons in a single

segment shown by a blue disk. (E) Neural activity with the optogenetic silencing of excitatory

neurons. Excitatory neurons in the A3 segment were silenced for 2 seconds, marked by a

blue bar. Waves were arrested after the optogenetic silencing. (F) Traces of segment length

in (E). Dotted lines denote the equilibrium length of the segments. In the later phase of the

optogenetic silencing (the shaded region), the length of all the segments returned to the

equilibrium length. (G) A schematic of optogenetic activation of inhibitory neurons in a single

segment shown by a red disk. (H) Neural activity with the optogenetic activation of inhibitory

neurons. Inhibitory neurons in the A3 segment were activated for 2 seconds, marked by a

red bar. Waves were arrested after the optogenetic activation. (I) Traces of segment length

in (H). Dotted lines denote the equilibrium length of the segments. In the later phase of the

optogenetic activation of inhibitory neurons (the shaded region), the length of all the

segments returned to the equilibrium length. Plot colours in B, C, E, F, H, and I correspond

to those in Figure 1F.

Figure 7. Mathematical simulation and experimental analysis of crawling behaviour in low friction conditions.

(A and B) Simulation results of kymograph in the optimized condition (A) and the absence of friction (B). (C and D) Simulation results of segmental length in the optimized condition (C) and the absence of friction (D). (E-H) Comparison of four kinematic parameters in simulations between in the optimized condition (Control) and the absence of friction (No friction). (E) Maximum segment length. (F) Minimum segment length. (G) Contraction duration. (H) Intersegmental delay. (I and J) Plots of segment length measured by the experiments of larvae on agarose (I) and those floating in liquid (J). (K-N) Comparison of four kinematic parameters obtained by the experiments of larvae on agarose (On agarose) and larvae in a low friction condition (Floating). The p-values show the result of Student's t-test. (K) Maximum segment length. (L) Minimum segment length. (M) Contraction duration. (N) Intersegmental delay.

Figure 8. Sensory feedback and central connectivity are both involved in controlling crawling speed.

(A) The weights of intersegmental proprioceptive sensory feedback w_{ES} and intersegmental coupling w_{En} in the neuromechanical model. (B and C) Simulation in the optimized condition. (B) Segmental boundary kymograph. (C) Activity of excitatory (red line), inhibitory (blue line), and sensory neurons (dotted lines) in a single segment. (D and E) Simulation in the absence of proprioceptive sensory feedback. (D) Segmental boundary kymograph. (E) Activity of excitatory (red line), inhibitory (blue line), and sensory neurons (dotted lines) in a single segment. (F and G) Simulation in the absence of intersegmental connections. (F) Segmental boundary kymograph. (G) Activity of excitatory (red line), inhibitory (blue line), and sensory neurons (dotted lines) in a single segment. (H and I) Plots of speed as proprioceptive sensory feedback w_{ES} (H) or intersegmental coupling w_{En} was perturbed (I). Grey shaded regions

976   show the range of speed observed in the experiment with third-instar larvae. Red dots

977   indicate the optimized simulation condition.

Figure 9. Interaction between w_{ES} and w_{En} in controlling crawling speed.

(A) Plots of segment displacement in varied combinations of proprioceptive sensory feedback w_{ES} (along the vertical axis) and intersegmental coupling w_{En} (along the horizontal axis). The plot enclosed in a black rectangle corresponds to the optimized condition. (B) A plot of speed as both proprioceptive sensory feedback w_{ES} and intersegmental coupling w_{En} were perturbed. A grey line and a shaded region show the average and the range of speed observed in the experiment with third-instar larvae, respectively.

Fig. 10. Intrasegmental excitatory and inhibitory connections are both involved in controlling crawling speed.

(A) The weights of intrasegmental connections between excitatory neurons (w_{EE}) and intrasegmental connections from inhibitory neurons to excitatory neurons (w_{EI}) in the neuromechanical model. (B and C) Simulation in the optimized condition. (B) Segmental boundary kymograph. (C) Activity of excitatory (red line), inhibitory (blue line), and sensory neurons (dotted lines) in a single segment. (D and E) Simulation in the absence of intrasegmental connections between excitatory neurons. (D) Segmental boundary kymograph. (E) Activity of excitatory (red line), inhibitory (blue line), and sensory neurons (dotted lines) in a single segment. (F and G) Simulation in the absence of intrasegmental connections from inhibitory neurons to excitatory neurons. (F) Segmental boundary kymograph. (G) Activity of excitatory (red line), inhibitory (blue line), and sensory neurons (dotted lines) in a single segment. (H and I) Plots of speed as the weight of intrasegmental

1002   connections between excitatory neurons w_{EE} (H) or the weight of connections from inhibitory

1003   neurons to excitatory neurons w_{EI} was perturbed (I). Grey shaded regions show the range of

1004   speed observed in the experiment with third-instar larvae. Red dots indicate the optimized

1005   simulation condition.

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Fig. 11. Interaction between w_{EE} and w_{EI} in controlling crawling speed.

(A) Plots of segment displacement in varied combinations of the weights of intrasegmental

connections between excitatory neurons w_{EE} (along the horizontal axis) and from inhibitory

neurons to excitatory neurons w_{EI} (along the vertical axis). The plot enclosed in a black

rectangle corresponds to the optimized condition. (B) A plot of speed as both w_{EE} and w_{EI}

were perturbed. A grey line and a shaded region show the average and the range of speed

observed in the experiment with third-instar larvae, respectively.

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Fig. 12. Prediction of the strength of intersegmental connections in sister species in

genus _Drosophila._

The black curve shows the relation between the intersegmental coupling w_{En} and crawling

speed obtained by the neuromechanical model based on the measurement of _Drosophila_

melanogaster larvae. This plot was obtained by averaging out the weight of proprioceptive

sensory feedback w_{ES} in Figure 9B. The average and standard error mean of speed in

species in the genus _Drosophila_ are shown by solid lines and shaded area, respectively. The

speed data was calculated from data in (57).

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 Supporting Information

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1031 **Supplementary Figure 1. A physical model with eleven segments.**

1032 Based on the estimation of the number of segments, the fly larva was modelled by eleven

1033 segments. We assumed that y_{10} and y_{-1} were physically coupled. In the simulation results

1034 in this paper, segmental boundaries from y_{10} to y_0 or segments from A8 to T2 were shown.

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1037　**Supplementary Figure 2. Fitting stress-relaxation test data by three viscoelastic**

1038　**models.**

1039　The same stress-relaxation test data was fitted with the SLS model (A), Maxwell model (B),

1040　and Kelvin-Voigt model (C).

1041

B From measurement

m	0.1 mg
k_1	40.7 mN/mm
k_2	58.3 mN/mm
c	2640 mN sec/mm
$\max M_i$	6.7 mN
L	0.35 mm

C From fitting

F_f	0.05 mN
μ_{bf}	10
w_{IE}	0.8
w_{EI}	-2
w_{ME}	540
w_{ES}	300
w_{IS}	300 (= w_{ES})
w_{EE}	2
w_{En}	0.6
θ_E	0.6
τ_E	35 msec
θ_I	0.6
τ_I	120 msec
θ_M	4.8
τ_M	40 msec
θ_S	0.76

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1043 **Supplementary Figure 3. Our physical model for larval crawling and its parameters.**

1044 (A) Schematic of the physical model for larval crawling. (B) List of parameters whose values

1045 were obtained by measurement using fly larvae. (C) List of parameters whose values were

1046 obtained by fitting to reproduce larval crawling by the simulation.

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Supplementary Figure 4. Perturbation analysis on viscoelasticity

Plots of speed as viscoelasticity was perturbed. (A) Perturbation of the spring constant k_1.
(B) Perturbation of the spring constant k_2. (C) Perturbation of the dumping coefficient c. The
horizontal axes were normalized by the optimized values ($k_{1\_optimal}$, $k_{2\_optimal}$, and
$c\_optimal$), respectively. Grey shaded regions show the range of speed observed in the
experiment with third-instar larvae. Red dots indicate the optimized simulation condition. The
minimum value in the horizontal axis in the plot of (C) equals 1/400, which corresponds to
the value in Pehlevan *et al.* (2016).

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1059 **Supplementary Figure 5. Perturbation analysis on the asymmetricity in friction**

1060 Plots of speed as the friction asymmetricity was perturbed. The grey shaded region shows

1061 the range of speed observed in the experiment with third-instar larvae. The red dot indicates

1062 the optimized simulation condition.

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Supplementary Figure 6. Perturbation analysis on the maximum muscular force

Muscular force and segment displacement when the maximum muscular contraction force

was perturbed. (A-D) Muscular forces in all the segments. Line colours correspond to those

in Figure 1B and 1C. (E-H) Displacement of the segmental boundaries. Line colours

correspond to those in Figure 1E and 1F. The ratio of the maximum contraction force to the

optimized force: A and E, 100%; B and F, 75%; C and G, 50%; D and H, 25%.

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Supplementary Figure 7. Different durations of optogenetic stimulation in the
simulation exhibit distinct phenotypes in the propagation of waves.

(A) Schematic of optogenetic silencing of excitatory neurons in a single segment shown by

a blue disk. (B) Neural activity with the optogenetic silencing of excitatory neurons. Excitatory

neurons in the A3 segment were silenced for 0.5 seconds, marked by a blue bar. Waves

were resumed just after the optogenetic silencing was removed. (C) Traces of segment

length in (B). The dotted box shows the segment length of the posterior neighbouring

segment during optogenetic stimulation. The arrow indicates that the neighbouring segment

was contracted just after the optogenetic stimulus was removed. (D) Neural activity with the

optogenetic silencing of excitatory neurons for 0.7 seconds. Excitatory neurons in the A3

segment were silenced as marked by a blue bar. Waves were arrested even after the

optogenetic silencing was removed. (E) Traces of segment length in (D). The dotted box

indicates the segment length of the posterior neighbouring segment during optogenetic

1086   stimulation. The arrow indicates that the neighbouring segment was returned to the

1087   equilibrium length just after the optogenetic stimulus was removed.

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1090 **Supplementary Figure 8. Frequency of crawling in a low friction condition.**

1091 (A) Comparison of crawling frequency between larvae on agarose and floating. (B)

1092 Comparison of crawling frequency in simulation between in the optimized condition (Control)

1093 and the absence of friction (No friction).

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