Cingulo-Opercular Control Network Supports Disused Motor Circuits in Standby Mode

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Abstract

Two weeks of upper extremity casting induced plasticity beyond somatomotor regions. Whole-

brain resting-state functional MRI (rs-fMRI) revealed that disused motor regions became more

strongly connected to the cingulo-opercular network (CON), an executive control network that

includes regions of the dorsal anterior cingulate cortex (dACC) and insula. Disuse-driven

increases in functional connectivity (FC) were specific to the CON and somatomotor networks

and did not involve any other networks, such as the salience, frontoparietal or default mode

networks. FC increases during casting were mediated by large, spontaneous activity pulses

that appeared in disused motor regions and network-adjacent CON control regions. During

limb constraint, disused motor circuits appear to enter a standby mode characterized by

spontaneous activity pulses and strengthened connectivity to CON executive control regions.

Introduction

Disuse is a powerful paradigm for inducing plasticity that has uncovered key organizing

principles of the human brain[1-4]. Monocular deprivation revealed that multiple afferent inputs

can compete for representational territory in the primary visual cortex[1]. Competition between

afferents also shapes the somatomotor system, and manipulations such as peripheral nerve

deafferentation, whisker trimming, and limb constraint all drive plasticity in the primary

somatosensory and motor cortex[2-4]. Most plasticity studies to date have used focal techniques,

such as microelectrode recordings, to study local changes in brain function. As a result, little is

known about how behavior and experience shape brain-wide functional networks.

The brain is composed of networks of regions that cooperate to perform specific cognitive

operations[5-7]. These functional networks show synchronized spontaneous activity while the

brain is at rest, a phenomenon known as resting state functional connectivity (FC)[8-10]. FC can

be measured non-invasively in humans using resting-state functional MRI (rs-fMRI). Whole-

brain rs-fMRI has been used to parse the brain into canonical functional networks[11,12],

including visual, auditory and somatomotor networks[13,14]; ventral and dorsal attention

networks[7,15]; a default mode network with roles in internally directed cognition and episodic

memory[6,10]; a salience network thought to assess the homeostatic relevance of external

stimuli[16]; a frontoparietal control network supporting error-processing and moment-to-moment

adjustments in behavior[17-19]; and a cingulo-opercular control network (CON), which maintains

executive control during goal-directed behavior[17,18,20].

A more recent advance in human neuroscience has been the recognition of individual

variability in network organization[21-24]. Most early rs-fMRI studies examined central tendencies

in network organization using group-averaged FC measurements[9,11,12]. Recent work has

demonstrated that functional networks can be described in an individual-specific manner if

sufficient rs-fMRI data are acquired, an approach termed Precision Functional Mapping

(PFM)[21,22,25-29]. PFM respects the unique functional anatomy of each person and avoids

averaging together functionally distinct brain regions across individuals.

We recently

demonstrated that PFM

can track disuse-driven

plasticity in the human

brain[30]. Three adult

participants (P1, P2 and

P3) were scanned at the

same time every day for

42-64 consecutive days

(30 minutes of rs-

fMRI/day) before, during

and after two weeks of

dominant upper extremity

casting (Fig. 1a-b).

During casting, the

upper-extremity regions

of the primary

somatomotor cortex (L-

SM1$_{ue}$) and cerebellum

Fig. 1 | Experimental Design and Spontaneous Activity Pulses. a, Three participants (P1, P2 and P3) wore casts covering the entire dominant upper extremity for two weeks. **b,** Participants were scanned every day for 42-64 consecutive days before, during and after casting. All scans included 30 minutes of resting-state functional MRI (rs-fMRI). **c,** During the cast period, disused somatomotor circuits exhibited spontaneous activity pulses[30].

(R-Cblm$_{ue}$) functionally disconnected from the remainder of the somatomotor network. Disused

motor circuits also exhibited large, spontaneous pulses of activity (Fig. 1c).

Somatomotor circuits do not function in isolation. Action selection and motor control are

thought to be governed by complex interactions between the somatomotor network and control

networks, including the CON[17]. Here, we leveraged the whole-brain coverage of rs-fMRI to

examine disuse-driven plasticity beyond the somatomotor system. We first examined disuse-

driven changes in FC between L-SM1$_{ue}$ and the remainder of the cerebral cortex. We then

performed comprehensive analyses of FC changes between all pairs of individual-specific

cortical, subcortical and cerebellar parcels (>200,000 possible connections). Finally, we tested

if observed changes in FC could be explained by the occurrence of spontaneous activity

pulses during the cast period.

Results

<u>**Disuse Caused Both Increases and Decreases in Functional Connectivity**</u>

To examine disuse-driven plasticity beyond somatomotor networks, we first generated seed

maps showing FC between L-SM1$_{ue}$ and all other cortical regions before, during and after

casting (Fig. 2a, Supplementary Fig. 1). Prior to casting (Pre), L-SM1$_{ue}$ was strongly connected

to the remainder of the somatomotor cortex (pre- and post-central gyri), especially homotopic

R-SM1$_{ue}$. During the cast period (Cast), L-SM1$_{ue}$ showed a new pattern of connectivity, with

strong connections to bilateral secondary somatosensory cortex (SII), dorsal anterior cingulate

cortex (dACC), and pre- and post-central sulci. After casting (Post), L-SM1$_{ue}$ FC returned to

baseline. Changes in FC during casting (Cast – Pre) and recovery (Post – Cast) were

examined using sets of previously published individual-specific cortical parcels[21,30]. Casting

caused decreased L-SM1$_{ue}$ connectivity with the remainder of the somatomotor cortex, as well

as increased connectivity with the bilateral SII, dACC, and pre- and post-central sulci (Fig. 2b, Supplementary Fig. 1). FC changes after cast removal were strongly negatively correlated with changes during casting (P1: spatial correlation, r = -0.56, P < 0.001; P2: r = -0.95, P < 0.001; P3: r = -0.32, P < 0.001), indicating that most effects reversed after cast removal (Fig. 2b, Supplementary Fig. 1).

Fig. 2 | Cast-driven Changes in Functional Connectivity (FC) of Disused Somatomotor Cortex (L-SM1ue). a, Seed maps showing FC between L-SM1ue and the remainder of the cerebral cortex in an example participant (P2; remaining participants, Supplementary Fig. 1). Seed maps were averaged across sessions before, during and after casting (Pre, Cast, Post). Labels indicate secondary somatosensory cortex (SII), dorsal anterior cingulate cortex (dACC), and pre- and post-central sulci (preCS and postCS). **b,** Subtraction maps showing changes in FC during casting (Cast – Pre) and recovery (Post – Cast). Differences are shown on a set of previously published individual-specific cortical parcels[21].

Disuse-driven Functional Connectivity Changes Were Highly Focal in Network Space

The brain's functional network organization can be visualized using spring-embedded graphs, which treat functional connections as spring forces, positioning more strongly connected nodes closer to one another (Fig. 3a, Supplementary Fig. 2). While L-SM1ue FC increases were

95 distributed in anatomical space, including regions on the medial and lateral surfaces of both

96 hemispheres, nearly all of these changes mapped onto a single cluster in network space, the

Fig. 3 | Disused Somatomotor Cortex (L-SM1ue) Functional Connectivity (FC) Changes in Network Space. **a,** Map of canonical functional networks in an example participant (P2; remaining participants, Supplementary Fig. 2). *Left:* Networks shown in anatomical space (inflated cortical surfaces). *Middle:* Same map as *Top*, shown in network space (spring-embedded graphs based on Pre scans). *Right:* Network color key: m-Vis: medial visual; l-Vis: lateral visual; Aud: auditory; f-SMN: face somatomotor; ue-SMN: upper-extremity somatomotor; le-SMN: lower-extremity somatomotor; CON: cingulo-opercular; FPN: fronto-parietal; Sal: salience; DAN: dorsal attention; VAN: ventral attention; MTL: medial temporal lobe; PMN: parietal memory; CAN: context association; DMN: default mode. **b,** *Left:* Subtraction maps showing disuse-driven decreases in functional connectivity (FC) with left somatomotor cortex (L-SM1ue) in anatomical space. *Middle:* Same map as *Top,* shown in network space. *Right:* Distribution of top 5% FC decreases across all networks. **P < 0.01; ***P < 0.001; FDR < 0.05. **c,** Subtraction maps showing disuse-driven increases in FC with L-SM1ue in anatomical (*Left*) and network space (*Middle*). *Right:* Distribution of top 5% FC increases across all networks.

CON (Fig. 3b, Supplementary Fig. 2). The network focality of L-SM1$_{ue}$ FC increases was

quantified by examining the distribution of the greatest FC increases (top 5%) across the

canonical functional networks (Fig. 3b). In all participants, the CON showed more FC

increases than expected by chance (P < 0.001 for all participants). Decreases in L-SM1$_{ue}$ FC

were also localized in network space (Fig. 3c, Supplementary Fig. 2). Most of the regions

showing decreased FC with L-SM1$_{ue}$ during casting belonged to the somatomotor networks

(ue-SMN, le-SMN, face-SMN and premotor). All participants showed more FC decreases than

expected by chance in the upper-extremity somatomotor network (ue-SMN; P < 0.001 for all

participants). Additionally, two participants (P2 and P3) showed significant FC decreases in

other somatomotor networks, including the lower-extremity and face somatomotor networks

(le-SMN and f-SMN) and the premotor network.

Plasticity Was Restricted to the Somatomotor and Cingulo-opercular Networks

The analyses presented thus far focus on changes in connectivity between L-SM1$_{ue}$ and the

remainder of the cerebral cortex. To examine whole-brain patterns of FC changes induced by

casting, we extracted rs-fMRI signals from individual-specific cortical, subcortical and

cerebellar parcels (P1: 744 parcels, P2: 733; P3: 761) and examined FC changes in all

possible pairwise connections (Supplementary Fig. 3). We displayed the 50 largest changes in

FC (25 greatest increases and 25 greatest decreases) in anatomical space (Fig. 4a,

Supplementary Fig. 3). Disuse-driven FC changes involved L-SM1$_{ue}$ more than expected by

chance (P1: 9/50 connections, P = 0.018; P2: 37/50, P < 0.001; P3: 39/50, P < 0.001). Figure

4b shows the total magnitude of

whole-brain FC change for each

vertex/voxel. The total magnitude

of whole-brain FC change was

significantly greater in L-SM1$_{ue}$

than in the remainder of the brain

(Fig. 4B, Supplementary Fig. 3;

P1: P = 0.021; P2: P < 0.001; P3:

P = 0.005).

Increased Somatomotor

Connectivity with the CON

Depended on a Recent History

of Disuse

To distinguish between increases

in connectivity due to wearing a

cast during MRI scans (i.e., an

altered behavioral state) and

increases in connectivity due to a

history of having been casted (i.e.,

disuse-driven plasticity), we

conducted a control experiment in

which participants wore casts

during 30-minute scans but were

not casted during their daily lives.

Fig. 4 | Whole-brain Analyses of Disuse-driven Functional Connectivity (FC) Changes. a, Changes in functional connectivity (FC) were computed for all pairs of cortical, subcortical and cerebellar parcels (mean Cast FC – mean Pre FC). The 50 most altered functional connections (top 25 increases, top 25 decreases) are shown for an example participant (P2; all participants, Supplementary Fig. 3). **b,** For each vertex/voxel, the magnitude of whole-brain FC change was computed as the sum of squared FC changes between that vertex and every other gray-matter vertex/voxel. Shown for an example participant (P2; all participants shown in Supplementary Fig. 4).

In both cases, we compared FC between L-

SM1$_{ue}$ and the left dorsal anterior cingulate

cortex (L-dACC; Fig. 5a), a key node of the

CON, in cast and no-cast conditions. As

suggested by the whole-brain network

analyses (Fig. 3b), FC between L-SM1$_{ue}$ and

L-dACC was significantly increased during

the cast period (Fig. 5b). When participants

wore casts during scans, but were not casted

during their daily lives, no changes in FC

were observed (Fig. 5c). This control

experiment indicated that increased FC

between the disused motor circuitry and the

CON depended on participants' recent

history of disuse, not their current state of

casting.

Network-Specific Connectivity Changes

Reflect Spontaneous Activity Pulses

Increases in FC with L-SM1$_{ue}$ showed a

similar anatomical distribution to the

spontaneous activity pulses we described

previously[30] (Fig. 6a-b). Additionally, FC

between L-SM1$_{ue}$ and the CON was highly

Fig. 5 | Connectivity between Disused Somatomotor Cortex and Cingulo-opercular Network during Disuse and Temporary Casting. a, Example regions of interest (ROIs) in the left primary somatomotor cortex (L-SM1$_{ue}$) and the left dorsal anterior cingulate cortex (L-dACC). **b,** Functional connectivity (FC) measured between L-SM1$_{ue}$ and L-dACC before (Pre), during (Cast) and after casting (Post). Two participants (P2 and P3) show a significant increase in FC during the cast period +P < 0.1, *P < 0.05, ***P < 0.001. (**C**) FC measured between L-SM1$_{ue}$ and L-dACC during both conditions of the control experiment: without casting (Off) and with temporary casts during scans (On). No changes in FC were observed.

167 correlated with the number of pulses detected in L-SM1$_{ue}$ during each scan (Fig. 6c; P1:

168   r=0.74, P<0.001; P2: r=0.57, P<0.001; P3: r=0.73, P<0.001). These observations led us to

169   suspect that FC between L-SM1$_{ue}$ and the CON was increased during the cast period because

170   both regions showed synchronized spontaneous activity pulses.

Fig. 6 | Relationship of Spontaneous Activity Pulses to Functional Connectivity (FC) Changes. a, Increases in FC with the disused somatomotor cortex (L-SM1$_{ue}$) during casting, repeated from Figure 3b for reference. **b,** Analysis of variance (ANOVA) showing regions with spontaneous activity pulses. ANOVA F-statistic was correlated with FC change in each parcel (P1: r = 0.16, P < 0.001; P2: r = 0.29, P < 0.001; P3: r = 0.06, P = 0.12). **c,** Relationship of FC between L-SM1$_{ue}$ and the dorsal anterior cingulate cortex (dACC; cingulo-opercular network (CON)) vs. the number of pulses detected. Each dot represents one 30-minute scan. Colored dots represent scans during the cast period. For all participants, FC between L-SM1$_{ue}$ and dACC was significantly correlated with the number of pulses detected (P1: r=0.74, P<0.001; P2: r=0.57, P<0.001; P3: r=0.73, P<0.001).

To test if spontaneous activity pulses could explain observed increases in FC, we implemented

a pulse censoring strategy, in which frames surrounding each detected pulse (13.2 s before –

17.6 s after each pulse peak) were excluded from FC calculations (Fig. 7a). This approach is

similar to the censoring strategy commonly used to

correct the effects of head-motion on FC[31].

Censoring pulses partially reduced the FC changes

observed during casting (Fig. 7b; P1 -55%, P = 0.14;

P2: -28%, P = 0.02; P3: -21%, P = 0.04; one-tailed t-

test). Additionally, the spatial pattern of FC changes

caused by pulse censoring (Censored – Uncensored;

Fig. 7c, Supplementary Fig. 4) was negatively

correlated with FC changes during casting (P1: r = -

0.35, P < 0.001; P2: r = -0.90, P < 0.001; P3: r = -33,

P < 0.001).

Censoring pulses did not entirely eliminate the effect

of casting on FC. The residual effect of casting after

pulse censoring was negatively spatially correlated

with the effects of pulse censoring (Supplementary

Fig. 4; P1: spatial correlation, r = -0.23, P < 0.001;

P2: r = -0.76, P < 0.001; P3: r = -0.18; P < 0.001),

suggesting that the residual effect may have been

driven by additional pulses that were too small to

distinguish from ongoing spontaneous activity

fluctuation. Pulses showed a wide distribution of

magnitudes (Fig. 8a; range: 0.4 – 1.2% rs-fMRI

signal change). Because pulses were detected using

a threshold-based approach[30], pulses smaller than

a Pulse censoring analysis

b Effect of pulse censoring on FC

c Effect of pulse censoring (Censored - Orig)

Fig. 7 | Censoring Pulses from Functional Connectivity (FC) Measurements. a, Schematic explaining censoring approach used to remove detected pulses from FC calculation. **b,** Censoring pulses partially reduced the difference between Pre and Cast scans. +P < 0.1, *P < 0.05, ***P < 0.001. **c,** Subtraction map showing reductions in L-SM1ue FC due to pulse censoring. The spatial pattern of FC changes due to pulse censoring was significantly negatively correlated with FC changes during casting (P1: r = -0.35, P < 0.001; P2: r = -0.90, P < 0.001; P3: r = -0.33, P < 0.001)

0.4% fMRI signal change

could not be detected and

censored. To test if smaller

pulses that escaped

detection could explain the

residual increased FC

between L-SM1$_{ue}$ and L-

dACC after pulse

censoring, we simulated a

full distribution of pulse

magnitudes by adding the

mean pulse time series

from L-SM1$_{ue}$ and L-dACC

to the baseline rs-fMRI

signals recorded from

these regions prior to

casting (Fig. 8b).

Simulated pulse

Fig. 8 | Addition of Simulated Pulses. a, Histogram of pulse magnitudes (peak fMRI signal), pooled across participants. A log-normal distribution (black line) was fit to the data using a least-squares approach. **b,** *Top:* Example resting-state functional MRI (rs-fMRI) signals from disused motor cortex (L-SM1$_{ue}$) and the dorsal anterior cingulate cortex (L-dACC) recorded prior to casting (Pre). *Bottom:* Same time series with simulated pulses added at random time points. Simulated pulse magnitudes were drawn from the full distribution shown in panel C. **c,** Adding simulated pulses increased FC between L-SM1$_{ue}$ and L-dACC (***P<0.001). Censoring simulated pulses partially reduced FC increases (***P<0.001). **d,** Subtraction map showing increases in L-SM1$_{ue}$ FC caused by simulated pulses in an example participant (P2; all participants, Supplementary Fig. 7).

magnitudes were drawn from a log-normal distribution, fit to the magnitude distribution of

detected pulses using a least-squares approach (Fig. 8a; see Supplementary Fig. 5 for

triangular and exponential distributions). Adding simulated pulses caused FC increases with a

similar effect size (P1: Δr = +0.07, P = 0.013; P2: +0.40, P < 0.001; P3: +0.19, P < 0.001) to

the FC increases observed during casting (Fig. 8c). Applying the same pulse censoring

strategy described above to the simulated pulses partially reduced the increases in FC (Fig.

8c; P1: -79%, P < 0.001; P2: -58%, P < 0.001; P3: -69%, P < 0.001), similar to the effect of

pulse censoring on the actual data (Fig. 7b). Adding simulated pulses to all brain regions,

using mean pulse time series specific to each region, recreated the anatomical distribution of

FC changes observed during casting (Fig. 7d, Supplementary Fig. 6; P1: r = 0.44, P < 0.001;

P2: r = 0.95, P < 0.001; P3: r = 0.64, P < 0.001). Thus, pulse with a full distribution of

magnitudes could account for observed FC changes during casting and the partial reversal of

FC changes after pulse censoring.

We also utilized the pulse censoring and pulse addition analyses to test if pulses could explain

observed decreases in FC within the somatomotor system. Pulse censoring did not

significantly reverse the decrease in FC between L-SM1$_{ue}$ and R-SM1$_{ue}$ observed during the

cast period (Supplementary Fig. 7). Adding simulated pulses to baseline time series decreased

FC between L-SM1$_{ue}$ and R-SM1$_{ue}$, but this effect was much smaller than that observed during

casting (Supplementary Fig. 7).

Discussion

Disuse Drives Plasticity of Functional Networks

Daily 30-minute scans of rs-fMRI before, during, and after casting revealed that disuse not only

causes plasticity within the primary motor cortex[3,30], but also increased functional connectivity

between disused circuits and executive control regions in the CON. These increases in FC

would have been difficult to observe using the focal recording techniques traditionally

employed to study plasticity. Thus, understanding the total impact of disuse on brain function

will require consideration of plasticity at multiple spatial scales. Future studies using positron

emission tomography (PET) to monitor local metabolic changes will further strengthen the

bridge between whole-brain plasticity and molecular mechanisms[32].

The high degree of network specificity seen in disuse-driven plasticity is a powerful

demonstration of the validity of individual-specific rs-fMRI network parcellations. It could have

been the case that casting produced a complex pattern of FC changes involving many brain

systems. Instead, we found that virtually all of the regions showing increased connectivity with

the disused motor cortex belonged to a single network, the CON. Large-scale functional

networks seem to be a fundamental unit of brain organization, important not only for

understanding patterns of activation during cognitive processes, but also for understanding

whole-brain patterns of plasticity.

Spontaneous Activity Pulses Alter Functional Connectivity

The network-specific increases in FC between the disused L-SM1$_{ue}$ and the CON likely reflect

the emergence of synchronized spontaneous activity pulses in these regions during casting.

FC is a measurement of the temporal correlation of spontaneous activity between brain

regions. Two complementary analyses (pulse censoring and pulse addition) suggested that

pulses contributed to increases in measured FC between disused motor regions and the CON.

Many studies have reported increased FC in neuropsychiatric conditions, e.g., Parkinson's

disease[33] and Major Depressive Disorder[34]. Perhaps some previously reported FC increases

could reflect spontaneous activity pulses, similar to those caused by limb disuse. Going

forward, spontaneous activity pulses, and the network-specific FC changes they produce,

could serve as a biP3ker of recent disuse and states of heightened plasticity[35].

Decreases in connectivity within the somatomotor system were not fully explained by

spontaneous activity pulses. Although the pulse addition analyses showed that spontaneous

activity pulses could contribute to decreases in connectivity observed during casting, both the

pulse censoring and pulse addition analyses suggested that at least part of the observed

decrease in connectivity occurred independently of pulses. Loss of typical co-activation of L-

SM1$_{ue}$ and R-SM1$_{ue}$ during daily behavior[30] likely contributed to casting-driven connectivity

decreases, consistent with the widely held hypothesis that FC is maintained by a Hebbian-like

mechanism that depends on co-activation of brain regions during behavior[18,32,36-38].

Disuse Impacts Cingulo-opercular Network (CON) Important for Executive Control

The importance of control systems in the human brain has been recognized for several

decades[5], but our understanding of these systems has changed dramatically over time and

continues to evolve[39]. Disentangling the roles of two functional networks mediating executive

control, the cingulo-opercular and frontoparietal networks, has relied largely on complex task

designs such as task-switching[20] and slow-reveal paradigms[40]. Here, we have demonstrated

that a new approach, whole-brain precision functional mapping combined with anatomically

specific disuse paradigms, can shed new light on the network interactions that support human

cognition and behavior. Although the brain contains several suspected cognitive control

networks beyond the CON, such as the frontoparietal (FPN), dorsal attention (DAN), ventral

attention (VAN) and salience (SAL) networks, disused motor regions only increased FC with

the CON. The CON is thought to initiate goal-directed behaviors and maintain executive

control settings in relation to task objectives[17,18]. The increased FC between disused L-SM1$_{ue}$

and the CON during casting suggests either 1) circuits within the CON were also disused

during casting, 2) the CON helps to maintain disused motor circuitry, or 3) spontaneous activity

pulses can spread along functional connections to neighboring brain regions in network space.

Spontaneous activity pulses may have emerged in the CON because its use was also reduced

during casting. We previously suggested that spontaneous activity pulses found in motor

regions may have been caused by disuse-driven changes in local inhibitory physiology[30,41].

The CON is generally thought to represent task sets, abstract parameters and motor programs

governing goal-driven behaviors[17,18]. Task sets can be applied to multiple motor effectors (e.g.,

right hand, left index finger, etc.), so it would be reasonable to think that casting one extremity

would not cause disuse of the CON. However, at least two sets of circuits within the CON may

have been disused during casting: circuits that represent bimanual behaviors and circuits that

convey task sets to effector-specific downstream regions (e.g., L-SM1$_{ue}$). During casting, many

of the task sets previously used to control the dominant upper extremity (e.g., inserting a key

into a lock) could have been used to control the non-dominant extremity. However, task sets

requiring bimanual coordination (e.g., fastening a belt) could not be applied to an alternative

set of motor effectors and may have become disused. Another set of CON circuits that may

have been disused are the circuits that convey task set information to effector-specific brain

regions. The CON contains both somatotopically organized regions (e.g., SMA, SII) and non-

somatotopic regions (e.g., anterior insula). Recent work shows that the SMA and SII, as well

as regions of the basal ganglia, may act as hubs that connect the rest of the CON to the

somatomotor network[26,42]. Such circuits could potentially undergo disuse during casting of one

extremity.

An alternative possibility is that inputs from the CON to L-SM1$_{ue}$ served a homeostatic function

during disuse, helping to maintain motor circuits that are typically maintained through active

use. We previously suggested that spontaneous activity pulses may help to maintain the

organization of disused brain circuits[30]. Perhaps pulses are triggered by the CON, which is the

system typically responsible for initiating activation of the somatomotor network[17].

Spontaneous activity pulses may also have originated in the disused somatomotor circuits and

spread along functional connections to brain regions that were not affected by casting. The

CON is immediately adjacent to the somatomotor network in network space (Fig. 3a). Previous

work in mice found that spontaneous activity bursts in somatosensory cortex, caused by local

pharmacogenetic suppression of inhibitory interneurons, spread to other functionally

connected regions not targeted by the experimental manipulation[43]. An interesting question for

future research is whether the CON would show spontaneous activity pulses following disuse

of brain systems other than the somatomotor network, such as networks supporting visual and

auditory processing, spatial navigation, or social cognition.

Two Complementary Mechanisms for Functional Network Plasticity

Extensive whole-brain imaging before, during and after casting revealed that disuse-driven

spontaneous activity pulses occur not only in primary motor and somatosensory areas, but

also in higher-order brain regions responsible for executive control over behavior (i.e., the

CON). The emergence of spontaneous activity pulses during casting produced increases in FC

that were highly focal in network space, specifically occurring between disused motor regions

and the CON. Decreases in connectivity between disused motor circuits and the remainder of

the somatomotor system, however, were not explained by spontaneous activity pulses. Thus,

disuse may drive network plasticity through two complementary mechanisms. Decreased

coactivation of brain regions during disuse might drive Hebbian-like disconnection between

disused and still-active somatomotor circuits. Spontaneous activity pulses, which contributed to

increased connectivity with the CON, may help preserve disused circuits for future

reintegration and use. Together, these two network plasticity mechanisms—Hebbian-like and

pulse-mediated—may represent a network-focal "stand-by mode" that allows the brain to

isolate disused circuits while simultaneously protecting them from premature functional

degradation.

Acknowledgements:
We thank Kristen M. Scheidter and Annie L. Nguyen for help in collecting MRI data and Ryan V. Raut for his comments on the manuscript. This work was supported by NIH grants NS110332 (D.J.N.), NS088590 (N.U.F.D.), TR000448 (N.U.F.D.), MH96773 (N.U.F.D.), MH122066 (N.U.F.D.), MH1000872 (T.O.L.), MH112473 (T.O.L.), NS090978 (B.P.K.), MH104592 (D.J.G.), NS080675 (M.E.R.), NS098577 (to the Neuroimaging Informatics and Analysis Center); the US Department of Veterans Affairs Clinical Sciences Research and Development Service grant 1IK2CX001680 (E.M.G.); Kiwanis Neuroscience Research Foundation (N.U.F.D.); the Jacobs Foundation grant 2016121703 (N.U.F.D.); the Child Neurology Foundation (N.U.F.D.); the McDonnell Center for Systems Neuroscience (D.J.N., T.O.L., A.Z., B.L.S., and N.U.F.D.); the McDonnell Foundation (S.E.P.), the Mallinckrodt Institute of Radiology grant 14-011 (N.U.F.D.); the Hope Center for Neurological Disorders (N.U.F.D., B.L.S., and S.E.P.).

Author Contributions:
D.J.N., T.O.L., C.R.H., A.Z.S., and N.U.F.D. designed the study. D.J.N., C.R.H., J.M.H., M.O., and N.U.F.D. collected the data. D.J.N. and E.M.G. analyzed the data. D.J.N., E.M.G., T.O.L., N.A.S., D.F.M., S.J.G., A.Z., A.N.N., B.A., A.R.C., B.P.K., D.J.G., M.E.R., S.E.P., A.Z.S., and N.U.F.D. interpreted the results. D.J.N. and N.U.F.D. wrote the manuscript with input from all other authors.

Declaration of interests:
The authors declare the following competing financial interest: N.U.F.D. is co-founder of NOUS Imaging.

METHODS

Human Participants

Participants were three healthy, adult volunteers. Details are described in Newbold *et al.*[30].

Experimental Intervention

We constrained the dominant upper extremity for two weeks by fitting each participant with a fiberglass

cast. Casts extended from just below the shoulder to past the fingertips. Details are described in

Newbold *et al.*[30].

MRI Acquisition

Participants were scanned every day of the experiment for 42-64 consecutive days. We collected 30

minutes of resting-state functional MRI (rs-fMRI) data every day of the experiment, as well as also task

fMRI and T1- and T2-weighted structural scans. Acquisition parameters and procedures are detailed in

Newbold *et al.*[30].

MR Image Processing

Preprocessing of structural and functional images, denoising of resting-state fMRI data, and cortical

surface projection were performed previously[30]. Fully processed data are available in the Derivatives

folder of the Cast-Induced Plasticity dataset on OpenNeuro (www.openneuro.org/datasets/ds002766).

ROI Selection

The region of the left primary somatomotor cortex controlling the casted upper extremity (L-SM1$_{ue}$) was

located individually in each participant using task fMRI. Details of the task analysis and region of

interest (ROI) selection are described in Newbold *et al.*[30]. The L-SM1$_{ue}$ ROI was used here to generate

seed maps (Fig. 2, Supplementary Fig. 1), to analyze spatial specificity of whole-brain functional

connectivity changes (Fig. 4b, Supplementary Fig. 3) and to measure FC between L-SM1$_{ue}$ and the

dorsal anterior cingulate cortex (dACC) for the removable cast control experiment (Fig. 5), the pulse

censoring analysis (Fig. 7) and the pulse addition analysis (Fig. 8, Supplementary Fig. 5).

Individual-specific sets of parcels spanning the entire cerebral cortex were previously generated for

each participant using a functional connectivity gradient-based approach, and each parcel was

assigned to one of 17 canonical functional networks using a graph theory-based community detection

algorithm[21,30]. Cortical parcels were used here to display functional connectivity changes in anatomical

(Fig. 2, 3, 6-8, Supplementary Fig. 1, 2, 4, 6) and network space (Fig. 3, Supplementary Fig. 2). We

also generated a set of subcortical and cerebellar parcels by assigning each voxel to the functional

network with which it showed the strongest functional connectivity and then grouping adjacent voxels

with matching network assignments into parcels. Sets of cortical, subcortical and cerebellar parcels

were used to examine changes in FC between all pairs of brain regions (Fig. 4, Supplementary Fig. 3).

A subset of parcels corresponding to the left primary somatomotor cortex (L-SM1$_{ue}$) was previously

generated by selecting all left-hemisphere parcels assigned to the upper-extremity somatomotor

network, excluding any parcels that fell outside of the pre- and post-central gyri[30]. Functional

connections between L-SM1$_{ue}$ parcels and all other parcels were averaged to generate parcel-wise

seed maps (Fig. 2, 3, 6-8, Supplementary Fig. 1, 2, 4, 6) and to quantify the spatial specificity of FC

changes between all cortical, subcortical and cerebellar parcels (Fig. 4, Supplementary Fig. 3).

Individual-specific ROIs in the left dorsal anterior cingulate cortex (L-dACC) were selected using pulse

analysis of variance (ANOVA) maps, which were previously generated for each participant[30]. ROIs

were selected within a large anatomical region, automatically labeled by FreeSurfer (union of caudal

anterior cingulate gyrus, posterior cingulate gyrus, and superior frontal gyrus). We first located the

vertex showing the maximum ANOVA F-statistic and then iteratively expanded the ROI by selecting

neighboring vertices in descending order of F-statistic, until the ROI included 100 vertices. The L-dACC

ROI was used to measure FC between L-SM1$_{ue}$ and the L-dACC for pulse censoring (Fig. 7) and pulse

addition analyses (Fig. 8, Supplementary Fig. 6).

Functional Connectivity Measurement

Mean rs-fMRI time series were extracted from the L-SM1$_{ue}$ ROI and each cortical, subcortical and

cerebellar parcel by averaging the time series of all vertices/voxels within the ROI/parcel. Vertex-wise

functional connectivity (FC) seed maps were generated for each session by computing a Pearson

correlation between the mean rs-fMRI time series from the $L\text{-}SM1_{ue}$ ROI and the time series from every

vertex. Frames with high head motion, identified previously[30], were excluded from FC calculations.

Vertex-wise seed maps were averaged across sessions before, during and after casting (Pre, Cast,

Post; Fig. 2, Supplementary Fig. 1).

FC between all pairs of cortical, subcortical and cerebellar parcels was measured as pairwise

correlations of all mean rs-fMRI time series, excluding high-motion frames, producing a correlation

matrix for each session. Correlation matrices were averaged over Pre, Cast and Post period. FC

changes during casting and recovery were computed as the differences between correlation matrices

(casting = Cast – Pre; recovery = Post – Cast). Full Cast – Pre differences matrices are shown in

Supplementary Figure 3. Parcel-wise difference seed maps showing changes in $L\text{-}SM1_{ue}$ FC during

casting and recovery (Fig. 2-3, Supplementary Fig. 1-2) were computed by averaging together columns

of the difference matrices corresponding to the $L\text{-}SM1_{ue}$ parcels (see *ROI selection,* above).

Spring Embedding

Cortical parcels were displayed in network space using force-directed ("spring-embedded") graphs[44],

generated with Gephi (https://gephi.org/). Graph weights were taken from parcel-wise correlation

matrices averaged across all sessions prior to casting (Pre). Graphs were thresholded to include only

the top 0.2% of pairwise functional connections. We initially examined graphs using an edge threshold

of 0.1%, but several parcels with large FC changes were disconnected from the main graph. Thus, we

selected the 0.2% connection threshold to display all key findings (Fig. 3, Supplementary Fig. 2).

Functional Connectivity Changes by Network

To test which functional networks showed large changes in FC with $L\text{-}SM1_{ue}$ during casting, parcel-wise

$L\text{-}SM1_{ue}$ seed maps were compared to individual-specific network maps. Parcel-wise $L\text{-}SM1_{ue}$

difference seed maps (Cast – Pre) were thresholded to contain the top 5% of parcels showing FC

increases/decreases. FC increases (Cast > Pre) and decreases (Cast < Pre) were examined

separately. The number of supra-threshold parcels in each cortical network is shown in Figure 3.

Alternative thresholds (top 1%, 10% and 20%) all yielded similar results. Networks containing a greater

number of FC increases/decreases than expected by chance were identified by comparing the number

of supra-threshold parcels found using each participant's true network map to the number of parcels

found using spatially permuted network maps (see *Statistical analyses*, below).

Whole-brain Analyses of Functional Connectivity Changes

The spatial specificity of whole-brain plasticity was examined by comparing changes in FC between all

cortical, subcortical and cerebellar parcels to individual-specific functional network maps. We examined

the top 50 changes in FC (25 greatest increases and 25 greatest decreases). A change in FC between

two parcels was counted as involving $L\text{-}SM1_{ue}$ if either of the two parcels was an $L\text{-}SM1_{ue}$ parcel. The

number $L\text{-}SM1_{ue}$ changes found using each participant's true network map was compared to the

number of $L\text{-}SM1_{ue}$ changes found using spatially permuted network maps (see *Statistical analyses*,

below).

To examine whole-brain FC changes at a finer spatial resolution, we examined differences in FC

between all cortical, subcortical and cerebellar vertices/voxels. We computed the magnitude of whole-

brain FC change between each vertex/voxel as the sum of squared FC changes between that

vertex/voxel and every other gray-matter vertex/voxel (Fig. 4, Supplementary Fig. 3). We tested if

whole-brain FC change was higher in $L\text{-}SM1_{ue}$ than in the rest of the brain by comparing the mean

magnitude of whole-brain FC change inside of each participant's true $L\text{-}SM1_{ue}$ ROI to the mean

magnitude of whole-brain FC change inside of spatially rotated ROIs (see *Statistical analyses*, below).

Spatial and Temporal Comparisons of Pulses and FC Changes

To generate a parcel-wise map of spontaneous activity pulses, we extracted rs-fMRI time series from

every cortical, subcortical and cerebellar parcel surrounding each detected pulse (13.2 seconds before

to 17.6 seconds after each pulse peak). Pulse peaks were detected previously[30]. We then performed an

ANOVA on the extracted time series (Fig. 6b). The spatial distribution of ANOVA F-statistics was

compared to the spatial distribution of L-SM1$_{ue}$ FC changes using a Pearson correlation across parcels.

We also compared the number of pulses detected during each rs-fMRI scan[30] to the FC measured

between L-SM1$_{ue}$ and L-dACC (Fig. 5c), using a Pearson correlation.

Pulse Censoring Analyses

To assess the contribution of large, detectable spontaneous activity pulses (>0.4% rs-fMRI signal

change) to FC changes observed during casting, frames surrounding each pulse (13.2 seconds before

to 17.6 seconds after each pulse peak) were excluded from FC calculations. Pulse detection criteria

were identical to those used previously [30]. We plotted FC measured between L-SM1$_{ue}$ and L-dACC

during each session before casting (Pre), during casting (Cast) and during casting with pulses excluded

(Cens; Fig. 7b). We compared Cast vs. Pre FC measurements and Cens vs. Cast FC measurements

using t-tests (see *Statistical analyses*, below). We also generated difference seed maps showing FC

changes between L-SM1$_{ue}$ and all cortical parcels due to censoring (Cens – Cast; Fig. 7c,

Supplementary Fig. 4).

Pulse Addition Analyses

To assess the contribution to FC changes of pulses with a hypothetical full magnitude distribution,

including pulses that were too small (<0.4% rs-fMRI signal change) to distinguish from ongoing

spontaneous activity fluctuations, we created simulated rs-fMRI time series containing a full distribution

of pulses. We first generated a histogram showing the magnitude distribution of detected pulses.

Magnitudes were grouped into bins with a width of 0.5%-signal-change. We then fit a log-normal

distribution to the observed pulse magnitudes using a least-squares approach (Fig. 8a). This provided

an estimate of the full pulse magnitude distribution, including pulses that were too small to detect. We

then added the mean pulse time series to the baseline (Pre) rs-fMRI time series, drawing pulse

magnitudes from the full log-normal distribution (example shown in Fig. 8b). The number of pulses

added was selected so that the number of large pulses (>0.4% signal change) would match the number

of pulses detected in each participant in an average Cast scan. We then computed FC of the baseline

time series (Pre) and the time series with added pulses (Sim; Fig. 8c). Finally, we applied the same

pulse censoring strategy described above to the simulated time series and computed FC after

censoring (Cens; Fig. 8c). Because pulse magnitudes were drawn from a full log-normal distribution,

only a portion of the added pulses were detected and censored. We compared Sim vs. Pre FC

measurements and Cens vs. Sim FC measurements using t-tests (see *Statistical analyses*, below). The

simulation and censoring procedures were repeated using triangular and exponential magnitude

distributions (Supplementary Fig. 5). We also generated difference seed maps showing FC changes

between L-SM1$_{ue}$ and all cortical parcels due to pulse simulation (Sim – Pre; Fig. 8d, Supplementary

Fig. 6).

Statistical Analyses

All statistical tests were performed identically for each participant. Whenever appropriate, we used

simple parametric statistical tests:

• Spatial similarity between anatomical maps was tested using a Pearson correlation across

parcels (P1: d.f. = 566; P2: 578; P3: 624). Spatial correlations were computed between the

following maps:

○ FC changes during casting (Cast – Pre) vs. FC changes during recovery (Post – Cast;

Fig. 2b)

○ FC changes during casting (Cast – Pre) vs. pulse ANOVA (F-statistic; Fig. 6)

○ FC changes during casting (Cast – Pre) vs. FC changes due to pulse censoring (Cens –

Cast; Fig. 7C, Supplementary Fig. 4)

○ FC changes due to pulse censoring (Cens – Cast) vs. residual FC changes after pulse

censoring (Cens – Pre; Supplementary Fig. 4)

○ FC changes during casting (Cast – Pre) vs. FC changes due to simulated pulses (Sim –

Pre; Fig. 8d, Supplementary Fig. 6)

- The number of pulses detected during each scan was compared to the FC measured between L-SM1$_{ue}$ and L-dACC using a Pearson correlation (P1: d.f. = 45; P2: 61; P3: 40; Fig. 6c).
- FC between L-SM1$_{ue}$ and L-dACC measured during each session of the cast period (P1: n = 13 sessions; P2: 13; P3: 14) was compared to FC during each session of the pre period (P1: n = 10; P2: 12; P3: 14) using a two-sided, unpaired t-test (P1: d.f. = 21, P2: 23, P3: 26; Fig. 7b).
- FC between L-SM1$_{ue}$ and L-dACC measured using the full time series (motion-censored only) of each session of the cast period (P1: n = 13 sessions; P2: 13; P3: 14) was compared to FC measurements of the same sessions excluding pulses (motion- and pulse-censored) using a one-sided, paired t-test (P1: d.f. = 24, P2: 24, P3: 26; Fig. 7b).
- FC between L-SM1$_{ue}$ and L-dACC measured during each session of the pre period (Pre; P1: n = 10; P2: 12; P3: 14) was compared to FC measurements of the same sessions after adding simulated pulses (Sim) using a two-sided, paired t-test (P1: d.f. = 18, P2: 22, P3: 26; Fig. 8c).
- FC between L-SM1$_{ue}$ and L-dACC measured using the full time simulated series (Sim; motion-censored only; P1: n = 10; P2: 12; P3: 14) was compared to FC measurements of the same sessions excluding pulses (motion- and pulse-censored) using a two-sided, paired t-test (P1: d.f. = 18, P2: 22, P3: 26; Fig. 8c).

When parametric statistical tests were not appropriate to test a specific hypothesis, we tested results against a null distribution generated via permutation resampling. In each case, our null hypothesis was that observed effects had no spatial relationship to ROIs/functional networks and any overlap occurred by chance. For vertex-wise ROIs, we modeled the null hypothesis by rotating the ROI around the cortical surface 1,000 times[45,46]. For functional networks, we modeled the null hypothesis by permuting the network assignments of parcels 1,000 times. Each permuted ROI/network map was used exactly as the actual map in order to compute a null distribution for the value of interest. The P-value reported for each test represents the two-sided probability that a value in the null distribution has a greater magnitude than the observed value. Permutation resampling was used to generate null distributions for the following values:

• Overlap of each functional network with increases in L-SM1$_{ue}$ FC during casting (Cast > Pre;

number of parcels in top 5%; Fig. 3b)

• Overlap of each functional network with decreases in L-SM1$_{ue}$ FC during casting (Cast > Pre;

number of parcels in top 5%; Fig. 3c)

• Overlap of L-SM1$_{ue}$ parcels with the 50 largest changes in FC between all pairs of cortical,

subcortical and cerebellar parcels (Fig. 4a, Supplementary Fig. 3)

• Magnitude of whole-brain FC change in the L-SM1$_{ue}$ ROI (Fig. 4b, Supplementary Fig. 3)

Since we tested the overlap of L-SM1$_{ue}$ FC increases/decreases with 17 different functional networks, a

Benjamini-Hochberg procedure was applied to correct for multiple comparisons, maintaining false

discovery rates < 0.05. Each of the three participants constituted a separate replication of the

experiment, rather than multiple comparisons, so no correction was necessary for tests repeated in

each participant.

Data Visualization

Regions of interest and whole-brain pulse maps were shown on cortical surfaces generated by

FreeSurfer[47] and Human Connectome Project (HCP) Workbench software packages[48]. These images

were rendered using HCP Workbench[48]. Figures showing the greatest differences in functional

connectivity across the entire brain in inflated anatomical space (Fig. 4, Supplementary Fig. 3) were

rendered using Blender, a free and open-source 3D modeling software package (www.blender.org). To

make the large number of changed connections included in these images visually compact,

connections following similar spatial trajectories were drawn toward each other using a previously

published mean-shift edge bundling algorithm[49]. All other figures were produced using Matlab

(www.mathworks.com).

Data Availability

This study used our previously published dataset[30], available on the OpenNeuro database

(www.openneuro.org/datasets/ds002766).

Code Availability

All code needed to reproduce our analyses is available on Gitlab

(https://gitlab.com/DosenbachGreene/cast-whole-brain).

a FC with disused somatomotor cortex (L-SM1ue)

b Changes in FC

Pre   Cast   Post

P1

Left Hemisphere

Right Hemisphere

L-SM1ue   FC (r)   0.1 ――― 0.6

Cast – Pre   Post – Cast

Δr   -0.15 ――― -0.05 +0.05 ――― +0.15

Pre   Cast   Post

P3

Left Hemisphere

Right Hemisphere

L-SM1ue   FC (r)   0.1 ――― 0.6

Cast – Pre   Post – Cast

Δr   -0.3 ――― -0.1 +0.1 ――― +0.3

Supplementary Fig. 1: Functional Connectivity (FC) Changes Involving the Disused Somatomotor Cortex (L-SM1ue) in Anatomical Space (All Participants). a, Seed maps showing FC between L-SM1ue and the remainder of the cerebral cortex in P1 (top) and P3 (bottom). Seed maps were averaged across sessions before, during and after casting (Pre, Cast, Post). **b,** Subtraction maps showing changes in FC during casting (Cast – Pre) and recovery (Post – Cast). Differences are shown on sets of 506 (P1) and 626 (P3) individual-specific cortical parcels. For P1 and P2, these parcels were previously generated and published (Gordon, 2017). We applied identical methods to generate a set of parcels for P3.

a Functional networks **b** L-SM1ue FC decreases **c** L-SM1ue FC increases

P1

Anatomical space

Gordon, *et al*, 2017

Network space

Δr
-0.15 ▬▬ -0.05

Δr
+0.1 ▬▬ +0.15

P3

Anatomical space

Network space

Δr
-0.3 ▬▬ -0.1

Δr
+0.1 ▬▬ +0.3

Supplementary Fig. 2: Functional Connectivity (FC) Changes Involving the Disused Somatomotor Cortex (L-SM1ue) in Anatomical and Network Space in P1 and P3.
a, Maps of 17 canonical functional networks in P1 (top) and P3 (bottom). Networks are shown in anatomical space (inflated cortical surfaces) and network space (spring-embedded graphs based on Pre scans). See Figure 3 for network color key. **b,** Subtraction maps showing disuse-driven decreases in functional connectivity (FC) with left somatomotor cortex (L-SM1ue) in anatomical space and network space. **c,** Subtraction maps showing disuse-driven increases in FC with L-SM1ue in anatomical and network space.

a Difference correlation matrices (Cast – Pre)

b Greatest FC changes (top 25 increases + top 25 decreases) in anatomical space

c Regions showing greatest FC changes

Supplementary Fig. 3: Whole-brain Patterns of Disuse-driven Plasticity. **a,** Matrices showing changes in functional connectivity (FC) between all pairs of individual specific cortical, subcortical and cerebellar parcels during casting (P1: 744 parcels, P2: 733; P3: 761**). b,** 50 largest changes in FC shown in anatomical space. **c,** Magnitude of whole-brain FC change, computed as the sum of squared FC changes between each vertex/voxel and every other gray-matter vertex/voxel

a Effect of pulse censoring (Cens - Cast)   **b** Residual effect (Cens - Pre)

P1

P2

P3

Δr   -0.1 ▮ +0.1   Δr   -0.1 ▮ +0.1

Δr   -0.2 ▮ +0.2   Δr   -0.2 ▮ +0.2

Δr   -0.2 ▮ +0.2   Δr   -0.2 ▮ +0.2

Supplementary Fig. 4: Functional Connectivity (FC) Changes Explained by Spontaneous Activity Pulses.
a, Subtraction map showing changes in L-SM1$_{ue}$ FC due to pulse censoring. The spatial pattern of FC changes due to pulse censoring was negatively correlated with FC changes during casting (P1: r = -0.35, P < 0.001; P2: r = -0.90, P < 0.001; P3: r = -33, P < 0.001). **b,** Subtraction map showing residual FC changes during casting after pulse censoring. The spatial pattern of residual FC changes was negatively correlated with the effect of pulse censoring (P1: spatial correlation, r = -0.23, P < 0.001; P2: r = -0.76, P < 0.001; P3: r = -0.18; P < 0.001).

a Exponential distribution

b Triangular distribution

Supplementary Fig. 5: Alternative Distributions for Pulse Magnitudes. a, Exponential distribution. *Left:* Histogram of pulse magnitudes (peak fMRI signal), pooled across all participants. An exponential distribution (black line) was fit to the data using a least-squares approach. *Right:* Adding simulated pulses, with magnitudes drawn from the exponential distribution, increased FC between L-SM1$_{ue}$ and L-dACC. Censoring simulated pulses partially reduced FC increases. *P<0.05, ***P<0.001. **b,** Triangular distribution. *Left:* Histogram of pulse magnitudes (peak fMRI signal), pooled across all participants. A linear distribution (black line) was fit to the data using a least-squares approach. *Right:* Adding simulated pulses, with magnitudes drawn from the linear distribution, increased FC between L-SM1$_{ue}$ and L-dACC. Censoring simulated pulses partially reduced FC increases. *P<0.05, **P<0.01, ***P<0.001.

Supplementary Fig. 6: Functional Connectivity (FC) Changes Caused by Simulated Spontaneous Activity Pulses (All Participants). a, Subtraction map showing changes in L-SM1$_{ue}$ FC due to addition of simulated pulses. FC changes due to pulse addition closely matched FC changes during casting (P1: spatial correlation, r = 0.44, P < 0.001; P2: r = 0.95, P < 0.001; P3: r = 0.64, P < 0.001). **b,** Subtraction map showing effect of censoring simulated pulses. Effects of censoring closely complemented the effect of pulse addition (P1: r = -0.71, P < 0.001; P2: r = -0.96, P < 0.001; P3: r = -0.69; P < 0.001).

a Left and right motor regions of interest

b Functional connectivity vs. number of pulses detected during each scan

c Effect of pulse censoring   ## d Effect of pulse addition

Supplementary Fig. 7: Functional Connectivity (FC) Decreases Were Not Explained by Spontaneous Activity Pulses. **a,** Example regions of interest (ROIs) in the left and right primary somatomotor cortex (L-SM1ue and R-SM1ue). **b,** Relationship of FC between L-SM1ue and R-SM1ue vs. the number of pulses detected. Each dot represents one 30-minute scan. Colored dots represent scans during the cast period. For all participants, FC between L-SM1ue and R-SM1ue was significantly correlated with the number of pulses detected (P1: r=0.74, P<0.001; P2: r=0.57, P<0.001; P3: r=0.73, P<0.001). **c,** Censoring pulses did not reduce the difference between Pre and Cast scans. ***P < 0.001. **d,** Adding simulated pulses decreased FC between L-SM1ue and R-SM1ue in two participants (P2 and P3), but these decreases were much smaller than those observed during casting. ***P < 0.001. **P < 0.01.

REFERENCES

Wiesel, T. N. & Hubel, D. H. Comparison of the effects of unilateral and bilateral eye closure on cortical unit responses in kittens. *J Neurophysiol* **28**, 1029-1040, doi:10.1152/jn.1965.28.6.1029 (1965).

Merzenich, M. M. *et al.* Topographic reorganization of somatosensory cortical areas 3b and 1 in adult monkeys following restricted deafferentation. *Neuroscience* **8**, 33-55 (1983).

Milliken, G. W., Plautz, E. J. & Nudo, R. J. Distal forelimb representations in primary motor cortex are redistributed after forelimb restriction: a longitudinal study in adult squirrel monkeys. *J Neurophysiol* **109**, 1268-1282, doi:10.1152/jn.00044.2012 (2013).

Feldman, D. E. & Brecht, M. Map plasticity in somatosensory cortex. *Science* **310**, 810-815, doi:10.1126/science.1115807 (2005).

Posner, M. I. & Petersen, S. E. The attention system of the human brain. *Annu Rev Neurosci* **13**, 25-42, doi:10.1146/annurev.ne.13.030190.000325 (1990).

Raichle, M. E. *et al.* A default mode of brain function. *Proc Natl Acad Sci U S A* **98**, 676-682, doi:10.1073/pnas.98.2.676 (2001).

Shulman, G. L., Ollinger, J. M., Linenweber, M., Petersen, S. E. & Corbetta, M. Multiple neural correlates of detection in the human brain. *Proc Natl Acad Sci U S A* **98**, 313-318, doi:10.1073/pnas.021381198 (2001).

Biswal, B., Yetkin, F. Z., Haughton, V. M. & Hyde, J. S. Functional connectivity in the motor cortex of resting human brain using echo-planar MRI. *Magn Reson Med* **34**, 537-541 (1995).

Fox, M. D. *et al.* The human brain is intrinsically organized into dynamic, anticorrelated functional networks. *Proc Natl Acad Sci U S A* **102**, 9673-9678, doi:10.1073/pnas.0504136102 (2005).

Greicius, M. D., Krasnow, B., Reiss, A. L. & Menon, V. Functional connectivity in the resting brain: a network analysis of the default mode hypothesis. *Proc Natl Acad Sci U S A* **100**, 253-258, doi:10.1073/pnas.0135058100 (2003).

Yeo, B. T. *et al.* The organization of the human cerebral cortex estimated by intrinsic functional connectivity. *J Neurophysiol* **106**, 1125-1165, doi:10.1152/jn.00338.2011 (2011).

Power, J. D. *et al.* Functional network organization of the human brain. *Neuron* **72**, 665-678, doi:10.1016/j.neuron.2011.09.006 (2011).

Cordes, D. *et al.* Frequencies contributing to functional connectivity in the cerebral cortex in "resting-state" data. *AJNR Am J Neuroradiol* **22**, 1326-1333 (2001).

Lowe, M. J., Mock, B. J. & Sorenson, J. A. Functional connectivity in single and multislice echoplanar imaging using resting-state fluctuations. *Neuroimage* **7**, 119-132, doi:10.1006/nimg.1997.0315 (1998).

Fox, M. D., Corbetta, M., Snyder, A. Z., Vincent, J. L. & Raichle, M. E. Spontaneous neuronal activity distinguishes human dorsal and ventral attention systems. *Proc Natl Acad Sci U S A* **103**, 10046-10051, doi:10.1073/pnas.0604187103 (2006).

Seeley, W. W. *et al.* Dissociable intrinsic connectivity networks for salience processing and executive control. *J Neurosci* **27**, 2349-2356, doi:10.1523/JNEUROSCI.5587-06.2007 (2007).

Dosenbach, N. U. *et al.* Distinct brain networks for adaptive and stable task control in humans. *Proc Natl Acad Sci U S A* **104**, 11073-11078, doi:10.1073/pnas.0704320104 (2007).

Dosenbach, N. U., Fair, D. A., Cohen, A. L., Schlaggar, B. L. & Petersen, S. E. A dual-networks architecture of top-down control. *Trends Cogn Sci* **12**, 99-105, doi:10.1016/j.tics.2008.01.001 (2008).

Marek, S. & Dosenbach, N. U. F. Control networks of the frontal lobes. *Handb Clin Neurol* **163**, 333-347, doi:10.1016/B978-0-12-804281-6.00018-5 (2019).

Dosenbach, N. U. *et al.* A core system for the implementation of task sets. *Neuron* **50**, 799-812, doi:10.1016/j.neuron.2006.04.031 (2006).

Gordon, E. M. *et al.* Precision Functional Mapping of Individual Human Brains. *Neuron* **95**, 791-807 e797, doi:10.1016/j.neuron.2017.07.011 (2017).

Laumann, T. O. *et al.* Functional System and Areal Organization of a Highly Sampled Individual Human Brain. *Neuron* **87**, 657-670, doi:10.1016/j.neuron.2015.06.037 (2015).

Wang, D. *et al.* Parcellating cortical functional networks in individuals. *Nat Neurosci* **18**, 1853-1860, doi:10.1038/nn.4164 (2015).

Mueller, S. *et al.* Individual variability in functional connectivity architecture of the human brain. *Neuron* **77**, 586-595, doi:10.1016/j.neuron.2012.12.028 (2013).

Marek, S. *et al.* Spatial and Temporal Organization of the Individual Human Cerebellum. *Neuron* **100**, 977-993 e977, doi:10.1016/j.neuron.2018.10.010 (2018).

Greene, D. J. *et al.* Integrative and Network-Specific Connectivity of the Basal Ganglia and Thalamus Defined in Individuals. *Neuron* **105**, 742-758 e746, doi:10.1016/j.neuron.2019.11.012 (2020).

Braga, R. M. & Buckner, R. L. Parallel Interdigitated Distributed Networks within the Individual Estimated by Intrinsic Functional Connectivity. *Neuron* **95**, 457-471 e455, doi:10.1016/j.neuron.2017.06.038 (2017).

Poldrack, R. A. *et al.* Long-term neural and physiological phenotyping of a single human. *Nat Commun* **6**, 8885, doi:10.1038/ncomms9885 (2015).

Sylvester, C. M. *et al.* Individual-specific functional connectivity of the amygdala: A substrate for precision psychiatry. *Proc Natl Acad Sci U S A* **117**, 3808-3818, doi:10.1073/pnas.1910842117 (2020).

Newbold, D. J. *et al.* Plasticity and spontaneous activity pulses in disused human brain circuits. *Neuron* **In press** (2020).

Power, J. D., Barnes, K. A., Snyder, A. Z., Schlaggar, B. L. & Petersen, S. E. Spurious but systematic correlations in functional connectivity MRI networks arise from subject motion. *Neuroimage* **59**, 2142-2154, doi:10.1016/j.neuroimage.2011.10.018 (2012).

Shannon, B. J. *et al.* Brain aerobic glycolysis and motor adaptation learning. *Proc Natl Acad Sci U S A* **113**, E3782-3791, doi:10.1073/pnas.1604977113 (2016).

Gratton, C. *et al.* Emergent Functional Network Effects in Parkinson Disease. *Cereb Cortex* **29**, 2509-2523, doi:10.1093/cercor/bhy121 (2019).

Greicius, M. D. *et al.* Resting-state functional connectivity in major depression: abnormally increased contributions from subgenual cingulate cortex and thalamus. *Biol Psychiatry* **62**, 429-437, doi:10.1016/j.biopsych.2006.09.020 (2007).

Kucyi, A. & Parvizi, J. Pupillary dynamics link spontaneous and task-evoked activations recorded directly from human insula. *J Neurosci*, doi:10.1523/JNEUROSCI.0435-20.2020 (2020).

Harmelech, T. & Malach, R. Neurocognitive biases and the patterns of spontaneous correlations in the human cortex. *Trends Cogn Sci* **17**, 606-615, doi:10.1016/j.tics.2013.09.014 (2013).

Guerra-Carrillo, B., Mackey, A. P. & Bunge, S. A. Resting-state fMRI: a window into human brain plasticity. *Neuroscientist* **20**, 522-533, doi:10.1177/1073858414524442 (2014).

Lewis, C. M., Baldassarre, A., Committeri, G., Romani, G. L. & Corbetta, M. Learning sculpts the spontaneous activity of the resting human brain. *Proc Natl Acad Sci U S A* **106**, 17558-17563, doi:10.1073/pnas.0902455106 (2009).

Petersen, S. E. & Posner, M. I. The attention system of the human brain: 20 years after. *Annu Rev Neurosci* **35**, 73-89, doi:10.1146/annurev-neuro-062111-150525 (2012).

Neta, M., Nelson, S. M. & Petersen, S. E. Dorsal Anterior Cingulate, Medial Superior Frontal Cortex, and Anterior Insula Show Performance Reporting-Related Late Task Control Signals. *Cereb Cortex* **27**, 2154-2165, doi:10.1093/cercor/bhw053 (2017).

Wellman, C. L., Arnold, L. L., Garman, E. E. & Garraghty, P. E. Acute reductions in GABAA receptor binding in layer IV of adult primate somatosensory cortex after peripheral nerve injury. *Brain Res* **954**, 68-72 (2002).

Gordon, E. M. *et al.* Three Distinct Sets of Connector Hubs Integrate Human Brain Function. *Cell Rep* **24**, 1687-1695 e1684, doi:10.1016/j.celrep.2018.07.050 (2018).

Rosenthal, Z. P. *et al.* Local Perturbations of Cortical Excitability Propagate Differentially Through Large-Scale Functional Networks. *Cereb Cortex* **30**, 3352-3369, doi:10.1093/cercor/bhz314 (2020).

Jacomy, M., Venturini, T., Heymann, S. & Bastian, M. ForceAtlas2, a continuous graph layout algorithm for handy network visualization designed for the Gephi software. *PLoS One* **9**, e98679, doi:10.1371/journal.pone.0098679 (2014).

Gordon, E. M. *et al.* Generation and Evaluation of a Cortical Area Parcellation from Resting-State Correlations. *Cereb Cortex* **26**, 288-303, doi:10.1093/cercor/bhu239 (2016).

Gordon, E. M. *et al.* Default mode network streams for coupling to language and control systems. *Proc Natl Acad Sci U S A* **In press** (2020).

Fischl, B. FreeSurfer. *Neuroimage* **62**, 774-781, doi:10.1016/j.neuroimage.2012.01.021 (2012).

Marcus, D. S. *et al.* Informatics and data mining tools and strategies for the human connectome project. *Front Neuroinform* **5**, 4, doi:10.3389/fninf.2011.00004 (2011).

Bottger, J., Schafer, A., Lohmann, G., Villringer, A. & Margulies, D. S. Three-dimensional mean-shift edge bundling for the visualization of functional connectivity in the brain. *IEEE Trans Vis Comput Graph* **20**, 471-480, doi:44E49295-068E-4AC0-9895-94C4713B93EC (2014).