

Synaptic diversity naturally arises from neural decoding of heterogeneous populations

Jacob L. Yates¹, Benjamin Scholl²

¹University of Maryland, College Park, Maryland, USA

²University of Pennsylvania, Department of Neuroscience, Perelman School of Medicine, Philadelphia, PA, USA

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Corresponding author: Benjamin Scholl, benjamin.scholl@pennmedicine.upenn.edu

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1 **Abstract**

2
3 The synaptic inputs to single cortical neurons exhibit substantial diversity in their sensory-
4 driven activity. What this diversity reflects is unclear, and appears counter-productive in
5 generating selective somatic responses to specific stimuli. We propose that synaptic diversity
6 arises because neurons decode information from upstream populations. Focusing on a single
7 sensory variable, orientation, we construct a probabilistic decoder that estimates the stimulus
8 orientation from the responses of a realistic, hypothetical input population of neurons. We provide
9 a straightforward mapping from the decoder weights to real excitatory synapses, and find that
10 optimal decoding requires diverse input weights. Analytically derived weights exhibit diversity
11 whenever upstream input populations consist of noisy, correlated, and heterogeneous neurons,
12 as is typically found *in vivo*. In fact, *in silico* weight diversity was necessary to accurately decode
13 orientation and matched the functional heterogeneity of dendritic spines imaged *in vivo*. Our
14 results indicate that synaptic diversity is a necessary component of information transmission and
15 reframes studies of connectivity through the lens of probabilistic population codes. These results
16 suggest that the mapping from synaptic inputs to somatic selectivity may not be directly
17 interpretable without considering input covariance and highlights the importance of population
18 codes in pursuit of the cortical connectome.

19 20 **Introduction**

21
22 Cortical neurons are driven by large populations of excitatory synaptic inputs. Synaptic
23 populations ultimately shape how sensory signals are encoded, decoded, or transformed. The
24 sensory representation or functional properties of an excitatory input population will define and
25 constrain the operations a neuron can perform and reflects the rules neurons use to form
26 connections. Electrophysiological and anatomical studies suggest that connections between
27 excitatory neurons exhibits functional specificity, where inputs are tuned for similar features as
28 the soma (Cossell et al., 2015; Ko et al., 2011; Lee et al., 2016; Reid and Alonso, 1995). In
29 contrast, synaptic imaging techniques have revealed that synaptic populations exhibit functional
30 diversity, deviating from canonical connectivity rules, such as 'like-connects-to-like' (Scholl and
31 Fitzpatrick, 2020). This functional diversity within input populations has been observed in a variety
32 of mammalian species, from rodents to primates, and for a variety of sensory cortical areas (Chen
33 et al., 2013, 2011; Iacaruso et al., 2017; Jia et al., 2011, 2010; Ju et al., 2020; Kerlin et al., 2019;

34 Scholl et al., 2017; Wertz et al., 2015; Wilson et al., 2018, 2016). This apparent discrepancy
35 challenges our understanding about how synaptic inputs drive the selective outputs of cortical
36 neurons and leads to a simple fundamental question: If the goal is to produce selective somatic
37 responses, why would a neuron have excitatory synaptic inputs tuned far away from the somatic
38 preference?

39 To answer this question, we turn to population coding theory; starting with the idea that to
40 accurately represent sensory signals, cortical neurons must decode the activity of upstream
41 populations. This decoding is likely accomplished by combing signals across neural populations
42 (Graf et al., 2011; Jazayeri and Movshon, 2006). Many studies have examined how sensory
43 variables might be decoded from cortical populations (Butts and Goldman, 2006; Graf et al., 2011;
44 Shamir and Sompolinsky, 2006), an endeavor increasingly applied to larger population sizes with
45 innovative recording techniques (Rumyantsev et al., 2020; Stringer et al., 2019). These decoding
46 approaches are often used as a tool to quantify the information about a stimulus available in a
47 neural population, carrying the assumption that downstream areas could perform such a process
48 (Berens et al., 2011; DiCarlo et al., 2012). In real brain circuits, decoders must be composed of
49 individual neurons, driven by sets of synaptic inputs, akin to a decoder's weights over a given
50 input population. To date, few studies have explicitly examined the weight structure of population
51 decoders (Jazayeri and Movshon, 2006; Rust et al., 2006; Zavitz and Price, 2019).

52 In this paper, we investigate the weights of a simple population decoder and how they
53 compare to real synaptic inputs measured *in vivo*. Focusing on a single sensory variable,
54 orientation, we derive the maximum-likelihood readout for a simulated input population that
55 encodes stimuli with noisy tuning curves (e.g., Ecker et al., 2011). Under reasonable assumptions,
56 the decoder weights can be interpreted as the synaptic connectivity between the input population
57 and the downstream decoder neurons. This allows us to examine how synaptic connectivity
58 depends on properties of the input population and to directly compare population decoders to
59 synaptic input measured *in vivo*. We then test a hypothesis that an optimal decoder will show
60 substantial heterogeneity in its synaptic weights given a biologically realistic input population. We
61 find that when input populations are shifted copies of the same tuning curve, the synaptic
62 excitatory inputs closely resemble the somatic output. However, with a biologically realistic input
63 population, the expected inputs onto readout neurons exhibit functional diversity. We then
64 compare the orientation tuning of simulated inputs with large populations of dendritic spines
65 (excitatory synaptic inputs) onto individual neurons of ferret primary visual cortex (V1), recorded
66 with two-photon calcium imaging *in vivo*. This comparison revealed similar diversity in the
67 orientation tuning of dendritic spines on ferret V1 neurons and simulated decoder weights. The

68 similarity between the synaptic populations of actual V1 neurons and the optimal neural decoder
69 suggest that diversity and heterogeneity observed in dendritic spines across sensory cortices are,
70 in fact, expected when considering how information is propagated through neural circuits in the
71 presence of noise.

72 Results

73
74
75 Following several decades of work on population coding theory, we derive a Bayesian
76 decoder to report the probability of a visual stimulus given inputs from a neural population (Fig.
77 1). With this framework, and given the specifics of the *encoding* population, we can analytically
78 derive the optimal *decoding* weights of a population of readout neurons. Here, we use “optimal”
79 to refer to the maximum-likelihood solution. Previous work has shown that a population of neurons

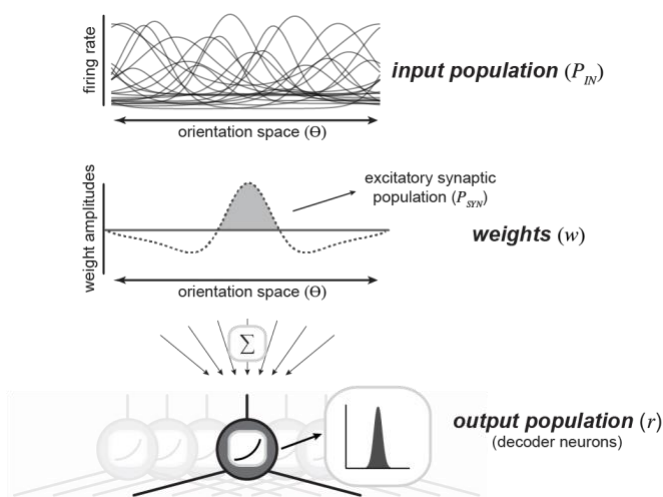


Figure 1: A population decoding framework to study synaptic diversity. An upstream population of neurons are tuned for a single stimulus variable (orientation) (*top*). This input population is readout by downstream decoder neurons (*bottom*). Downstream neurons decode stimulus identify by reading out spikes from the upstream input population. Each decoder neuron is defined by a set weights (*middle*) over the upstream population, which are summed and rectified to produce an output.

80 could perform such probabilistic decoding with weighted summation and divisive normalization,
81 as long as their inputs exhibit Poisson-like noise (Jazayeri and Movshon, 2006; Ma et al., 2006).
82 Starting from that basic framework, we derived a decoder that represents the probability that each
83 possible stimulus orientation was present given the responses of a large population of upstream,
84 input neurons (P_{IN}). This is effectively a categorical decoder, where each possible orientation is a
85 different category. Similar decoders have been used throughout the literature to estimate how
86 much information is in a neural recording and suggest how downstream neurons might read it out
87 (Graf et al., 2011; Stringer et al., 2019). Our decoder has weight vectors for each possible stimulus

88 orientation, which integrate across P_{IN} and are passed through a static nonlinearity (the
89 exponential function) and normalized. As we will show below, given specific assumptions about
90 the variability in P_{IN} , the weights over P_{IN} depend systematically on the tuning functions and
91 covariance of P_{IN} . Following a characterization of this decoding framework, we will make direct
92 comparisons with real data: defining an effective "synaptic input population" (P_{SYN}) as nonzero,
93 positive weights over P_{IN} . Although our strategy applies to any one-dimensional stimulus variable,
94 we describe this model in the context of orientation of drifting gratings presented to V1 neurons
95 for a direct comparison with *in vivo* measurements.

96

97 *A neural population as a probabilistic decoder*

98

99 A categorical probabilistic decoder reports the probability that a particular stimulus
100 orientation, θ_k , was present given the spiking responses of an input population, \mathbf{R} . This can be
101 expressed as a normalized exponential function of the log-likelihood plus the log prior for each θ_k ,

$$102 \quad p(\theta_k | \mathbf{R}) = \frac{p(\mathbf{R} | \theta_k) p(\theta_k)}{\sum_i p(\mathbf{R} | \theta_i) p(\theta_i)} = \frac{e^{L(\theta_k)}}{\sum_i e^{L(\theta_i)}}$$

103 where

$$104 \quad L(\theta_k) = \ln(p(\mathbf{R} | \theta_k)) + \ln(p(\theta_k))$$

105 The likelihood, $p(\mathbf{R} | \theta_k)$, is the probability of the observed responses in an input population given
106 the stimulus k and $p(\theta_k)$ is the prior probability of that stimulus class. If $p(\mathbf{R} | \theta_k)$ is in the exponential
107 family, then $L(\theta_k)$ can be written as a weighted sum of the input population response vector plus
108 an offset, which can be estimated numerically via multinomial logistic regression (Ma et al., 2006).
109 For simplicity, we assume the input population has a response that is a function of the stimulus
110 plus Gaussian noise, and equal covariance across all stimulus conditions. Although this
111 assumption about the covariance structure deviates from real neural activity, this assumption
112 means the weights and offset can be solved analytically (see Methods), and as will be shown
113 below, such a simple model makes substantial headway in explaining biological phenomena. Our
114 goal here is to provide a plausible alternative to "somatic selectivity" for the connectivity rules in
115 cortex. Under the Gaussian assumption, the decoder amounts to:

$$116 \quad p(\theta_k | \mathbf{R}) = \frac{e^{(\mathbf{R}^T \mathbf{w}_k + \beta_k)}}{\sum_{i=1}^K e^{(\mathbf{R}^T \mathbf{w}_i + \beta_i)}} \quad (1)$$

117 where

$$118 \quad \mathbf{w}_k = \mathbf{Q}^{-1} f(\theta_k)$$

119
$$\beta_k = -\left(\frac{1}{2}\right) f(\theta_k)^T Q^{-1} f(\theta_k) + \ln p(\theta_k)$$

120 Here, $f(\theta_k)$ is the mean input population response to stimulus orientation, k , K is the total number
121 of orientations, and Q is the covariance matrix. The covariance term captures the influence of
122 each neuron's response variance (diagonal elements) and the variability shared with other
123 neurons (off-diagonal elements). Intuitively, in the absence of covariability (i.e., off-diagonal
124 elements are zero), the weights are proportional to the signal-to-noise ratio of the neuron (the
125 mean divided by the variance). The term $\mathbf{R}^T w_k$ is the dot product between the population response
126 and weights. The second term, β_k , is an offset for each stimulus. $\ln p(\theta_k)$ is a constant reflecting
127 the log prior probability of stimulus k . It is worth noting that if the covariance depends on the
128 stimulus, the optimal readout is no longer a linear function of \mathbf{R} and is quadratic, which can be
129 interpreted as a complex-cell (Jaini and Burge, 2017; Pagan et al., 2016) and is a potentially
130 fruitful future direction.

131 In this study, we focus on the weights of this simple Gaussian, equal covariance decoder
132 in order to examine how synaptic tuning from such a simple decoder would arise. Because the
133 optimal weights have an analytic solution (eq. 1), we can see how they depend on the parameters
134 of P_{IN} . The simplifying assumptions we use to derive the maximum-likelihood weights help build
135 intuitions about what can be expected in biological circuits, and linear weights such as these could
136 be learned by real neural systems (Dayan and Abbott, 2001). A key difference here from prior
137 work is that rather than focus on discrimination (Haefner et al., 2013), we treat orientation
138 estimation as a multiclass identification problem, discretizing θ such that for each possible θ_k ,
139 there is a separate weight vector. Thus, in this derivation, the optimal weights depend on the
140 tuning curves themselves, not the derivative.

141

142 *Characteristics of a neural population decoder*

143

144 To understand how synaptic weights depend on input statistics, we derived maximum-
145 likelihood weights for input populations, P_{IN} , with different tuning and covariance. To generate P_{IN}
146 we simulated N neurons responding to K oriented stimuli ($\theta = [-90^\circ:K/180:+90^\circ]$). We briefly
147 describe the construction of P_{IN} here (full details are described in the Methods). Each neuron is
148 defined by a tuning function and noise term, describing trial-by-trial variability, which are summed
149 to generate stimulus-driven responses. We compared two fundamentally different types of input
150 populations that have been used in the literature, homogeneous and heterogenous, as well as
151 the role of correlated variability in shaping readout weights. A homogeneous P_{IN} consists of shifted

152 copies of a single tuning curve (Fig. 2a). Heterogenous P_{IN} have diverse tuning functions and
 153 were generated to match measurements from macaque V1 (Ringach et al., 2002). The
 154 heterogenous P_{IN} consisted of tuning curves closely resembling V1 physiology in terms of the
 155 variation in peak firing rate, bandwidth, and baseline firing rate (Fig. 2d). Varying amounts of
 156 limited-range correlations were included such that the noise correlation between two neurons

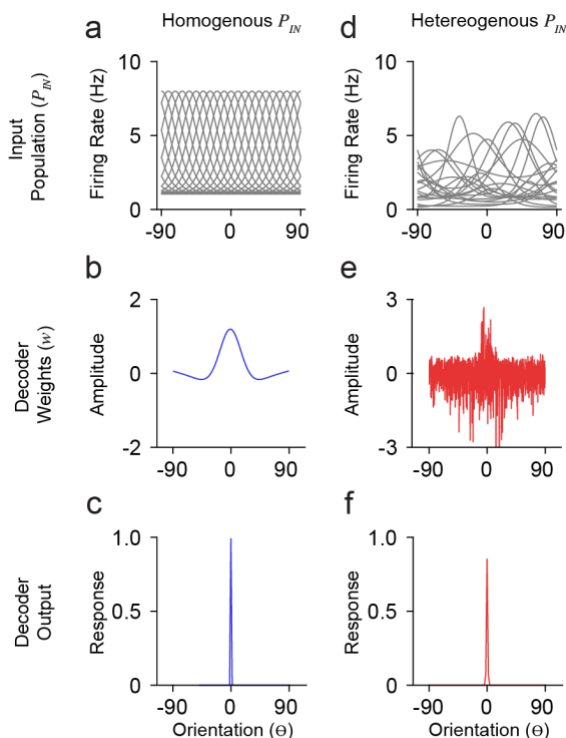


Figure 2: Model simulations with homogenous and heterogeneous input populations.

(a) Orientation tuning of a homogenous input population. Shown is a subset of the total population ($n = 20/1000$). Ordinate is orientation preference, restricted between -90° and 90° . (b) Derived weights for a single decoder neuron (preferring 0°) reading out the homogenous (blue) input population in (a). Weights for homogenous populations smoothly vary over orientation space. (c) Response output of the decoder neuron whose weights are shown in (b). (d-f) Same as in (a-c) for a heterogeneous input population with moderate correlation ($c_o = 0.25$). Note that decoder weights for heterogeneous input populations are not smooth.

157 depends on the difference in their tuning preferences (Ecker et al., 2011; Kohn et al., 2016).

158 The statistics of P_{IN} responses, \mathbf{R} , will dictate the weight structure for neurons in a decoding
 159 population. For a homogeneous P_{IN} , the weights are smooth across orientation space and exhibit
 160 three primary features: a prominent peak about the preferred orientation of the output tuning,
 161 slight negative weights for orientations just outside the preferred, and near-zero weights at
 162 orthogonal orientations (Fig. 2c). With more realistic tuning diversity (heterogenous P_{IN}), optimal
 163 weights are no longer smooth (Fig. 2d-e). While the optimal weights appear to roughly have the
 164 same overall shape as for homogeneous P_{IN} , there is considerable positive and negative

165 weighting across orientation space. Despite substantial changes in optimal weight vectors, the
 166 decoder output (i.e. somatic response) tuning was narrow (Fig. 2f), similar to the output for the
 167 homogeneous case (Fig. 2e).

168 To explore the importance of decoding weight diversity, we imposed a smoothing penalty
 169 on weight vectors (Park and Pillow, 2011). We calculated cross-validated decoder accuracy using
 170 the mean-squared error between the maximum a posteriori estimation and true stimulus (see
 171 Methods). Different degrees of smoothing are shown for an example set of weights in Figure 3a.
 172 We simulated a range of population sizes ($N = 2 - 2048$) and correlations ($c_o = 0, 0.25, 0.50$).

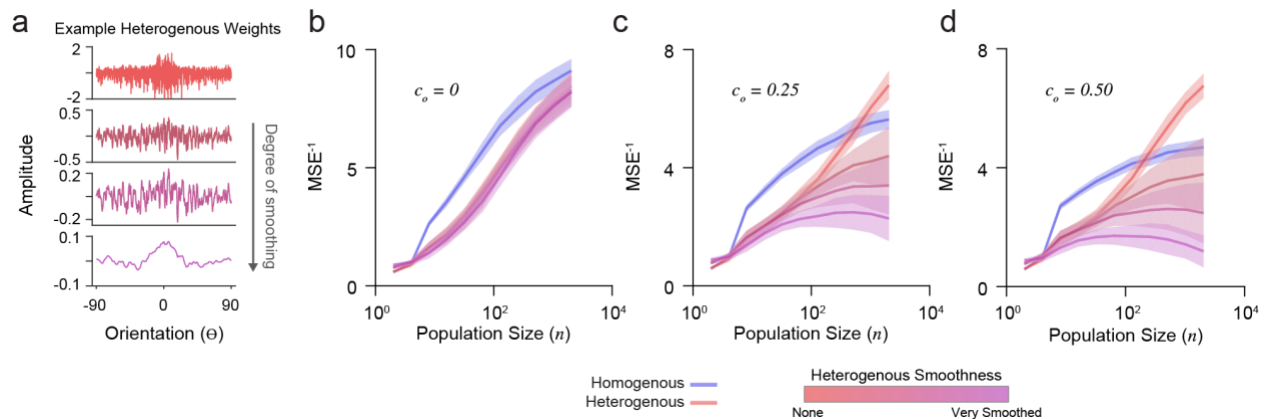


Figure 3: Decoder performance of heterogeneous input populations depends on population size, correlations, and weight diversity. (a) Example weight distribution for a decoder neuron reading out a heterogeneous input population (top). Shown are the effects of progressively smoothing weights. Smooth parameters (see Methods) from top to bottom: (0,0), (0.1,1), (0.2, 2), (1,10). Ordinate is orientation preference, restricted between -90° and 90° . (b) Decoder performance (inverse mean-squared-error) plotted for homogenous and heterogeneous input populations of increasing size. Simulations here include no correlations ($c_o = 0$). Shading indicates standard error. (c) Same as in (b) for input populations with moderate correlation ($c_o = 0.25$). (d) Same as in (b) for input populations with stronger correlation ($c_o = 0.50$).

173 Without noise-correlations, the accuracy of all decoders increases with population size,
 174 with a homogenous P_{IN} performing best (Fig. 3b). In the presence of noise-correlations, accuracy
 175 saturates for large homogenous P_{IN} (Fig. 3c-d). As previously shown (Ecker et al., 2011), accuracy
 176 for heterogeneous populations with limited-range correlations does not saturate (Fig. 3c-d).
 177 However, this depends on weight diversity. Smoothing the weights for heterogeneous P_{IN} caused
 178 saturation and decreased accuracy (Fig. 3c-d), demonstrating that weight amplitude diversity in
 179 analytically derived weights distributions are critical for the decoder performance.

180

181 *Simulating excitatory weight tuning*

182

183 In order to compare analytically derived weights with the synaptic inputs onto V1 neurons
184 measured *in vivo*, we generated excitatory synaptic input populations (P_{SYN}). Under the
185 assumption that synaptic integration is linear, two synapses of equal weight are the same as one
186 synapse with double that weight. This creates a degeneracy where synapse count and size trade
187 off. Because current spine imaging techniques typically capture large synapses and there is no
188 relationship between strength and orientation preference (Scholl et al., 2021), we can assume
189 size is fixed and convert the derived weights into a frequency distribution of ‘synaptic inputs’ (Fig.
190 4a). The tuning curve for such a synapse is the tuning curve of the input and thus, the synaptic
191 input population, P_{SYN} , is the input population resampled with probabilities given by the derived
192 weights. An example P_{SYN} for a single decoder neuron is shown in Figure 4b (drawn from the
193 heterogeneous P_{IN} in Figure 2). P_{SYN} in this example displays some specificity in orientation tuning
194 relative to the somatic output, indicated by a larger proportion of simulated synapses with similar
195 orientation preference as the somatic output (0°) of the decoder neuron.

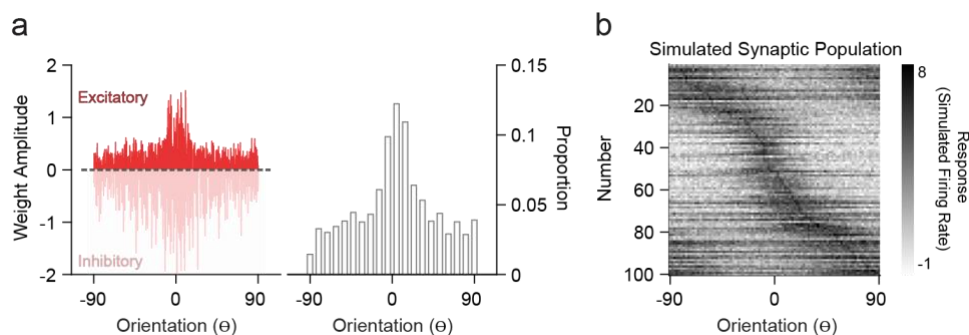


Figure 4: Simulation of synaptic populations from decoder neuron weight distributions. (a) Example weight distribution for a single decoder neuron tuned to 0° (left). Ordinates are orientation preference, restricted between -90° and 90° . Dashed line separates excitatory (positive) and inhibitory (negative) weights. Excitatory weight distribution over the input population is transformed into a frequency distribution, whereby greater amplitude equates to greater frequency of occurrence (right). (b) Example simulated synaptic population ($n = 100$ spines) from the weight distribution in (a). Shown are the orientation tuning curves of each simulated synapse (normalized).

196
197 *Empirical distribution of dendritic spine tuning is consistent with decoding of a heterogeneous*
198 *input population*

199 We analyzed two-photon calcium recordings from soma and corresponding dendritic
200 spines on individual neurons in ferret V1 during the presentation of oriented drifting gratings (see
201 Methods). While our model draws from a P_{IN} matched to measurements from macaque V1, the
202 orientation tuning of layer 2/3 neurons in ferret V1, as measured by two-photon cellular imaging,
203 exhibit a similar range in selectivity (Wilson et al., 2017). Visually responsive and isolated dendritic
204 spines (see Methods) typically exhibit diverse orientation tuning relative to the somatic output,

205 although some individual cells show greater overall diversity (Fig. 5b) than others (Fig. 5a). To
 206 characterize P_{SYN} diversity, both for real dendritic spines and simulated inputs, we computed the
 207 Pearson correlation coefficient between the tuning curves of individual inputs and the
 208 corresponding somatic output (Scholl et al., 2021). For these comparisons, we sampled
 209 orientation space in the model spines to match our empirical measurements (22.5 deg
 210 increments) and the number of total excitatory inputs recovered for each simulated downstream
 211 neuron was set to 100, similar to the average number of visually-responsive spines recorded for

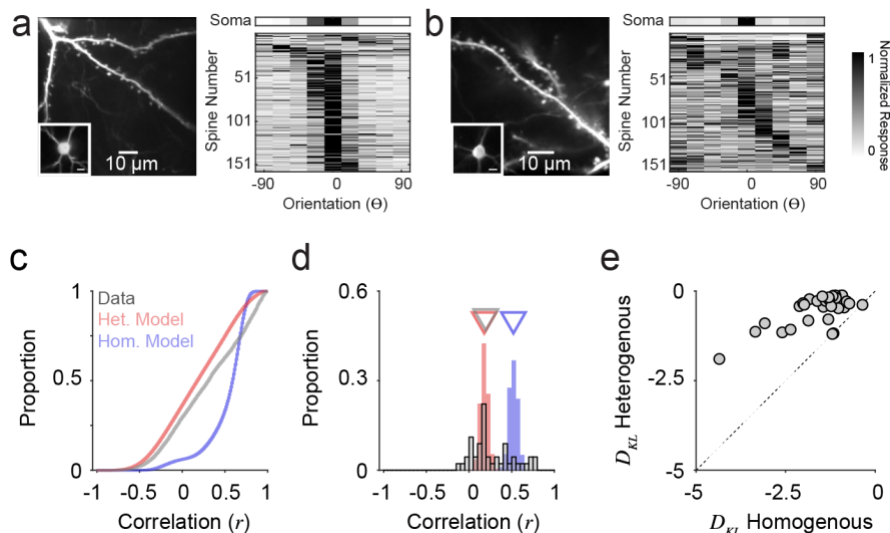


Figure 5: Orientation tuning diversity of dendritic spine populations in ferret V1 match simulations with correlated, heterogeneous input populations. (a) Two-photon standard-deviation projection of example dendrite and spines recorded from a single cell (*left*). Inset: Two-photon standard-deviation projection of corresponding soma. Scale bar is 10 microns. Orientation tuning of soma (*top*) and all visually-responsive dendritic spines from this single cell ($n = 159$) are shown (*right*). Spine responses are normalized peak $\Delta F/F$. Orientation preferences are shown relative to the somatic preference (aligned to 0°). (b) Same as in (a) for another example cell ($n = 162$ visually-responsive spines). (c) Cumulative distributions of tuning correlation between individual dendritic spines or simulated synaptic inputs with corresponding somatic tuning or decoder output. Shown are correlations of simulations of homogenous (*blue*) or heterogeneous (*red*) input populations, compared to empirical data (*gray*). (d) Distributions of average tuning correlation between synaptic input and somatic output across measured cells ($n = 45$). Also shown are distributions of average tuning correlation for simulated cells. Triangles denote median values for each distribution. (e) Comparison of Kullback-Leibler divergence (D_{KL}) between data and each model type. Each data point represents an individual cell's population of dendritic spines.

212 each ferret V1 neuron ($n = 45$, $n = 158.9 \pm 73.2$ spines/cell). Simulations were run 10,000 times,
 213 with $N = 1,000$ for P_{IN} and $c_o = 0.20$.

214 Across all simulated inputs, input-output tuning correlation was higher for homogeneous
 215 P_{SYN} compared to heterogeneous P_{SYN} (median $r_{hom} = 0.60$, median $r_{het} = 0.18$, $n = 900,000$; Fig.
 216 5c). Tuning correlation between all imaged dendritic spines and soma was low (median $r_{cell} =$

217 0.31, $n = 7,151$ spines from 45 cells), more closely resembling our model with a heterogeneous
218 P_{IN} . As somatic orientation selectivity (i.e., tuning bandwidth) varies for single cells in ferret V1
219 (Goris et al., 2015; Wilson et al., 2016), we next examined the average input-output tuning
220 correlation across individual cells (Fig. 5d). Here, the homogeneous model exhibited greater
221 specificity than the heterogeneous model (median $r_{hom} = 0.52$; median $r_{het} = 0.18$, $n = 90,000$). For
222 ferret V1 cells, we observed similar spine-soma correlation as the heterogeneous simulation
223 (median $r_{cell} = 0.20$, $n = 45$). Ferret V1 cells were not statistically different from neural decoders
224 with a heterogeneous P_{SYN} ($p = 0.19$, Mann-Whitney test), while neural decoders with a
225 homogeneous P_{SYN} were significantly more correlated with the inputs ($p < 0.0001$, Mann-Whitney
226 test). A small percentage of imaged cells (17.9%, $n = 5/28$) had synaptic populations whose mean
227 tuning correlation were within the 95% confidence interval of the homogeneous model distribution.
228 Additionally, some cells had negative average correlations with their spines, which never occurred
229 in the models—potentially indicating nonlinearities between the spines and soma. It is also
230 important to emphasize that both synaptic populations and the heterogeneous model exhibit a
231 positive bias in tuning correlations, illustrating that while inputs are functionally diverse, they are,
232 on average, more similarly tuned to the cell/decoder output.

233 Given the differences between ferret V1 neurons, we quantified the degree to which
234 synaptic populations on *each* neuron matched tuning correlation distributions from models of
235 homogeneous and heterogeneous P_{IN} , by calculating the Kullback-Leibler divergence (D_{KL} , bin size
236 = 0.05, see Methods). Across our population, imaged neurons more closely resembled
237 simulations with heterogeneous, compared to homogeneous, P_{IN} (93.3%, $n = 42/45$; Fig. 5e) and D_{KL}
238 from a heterogeneous model was consistently larger ($p < 0.0001$, sign rank Wilcoxon test). This
239 trend held for a range of histogram bin sizes (0.001 – 0.20). Importantly, the models are not fit to
240 data. They are derived entirely from the statistics of the input population, so this correspondence
241 between the heterogeneous model and the data results from no free parameters.

242 In addition to the similarity in input-output tuning correlation, we observed several trends
243 predicted by the heterogeneous model that were evident in synaptic populations imaged *in vivo*.
244 Simulated excitatory inputs correlated with the decoder output were not more selective for
245 orientation (see Methods) (bootstrapped PCA slope = 0.001 ± 0.004 s.e., $n = 10,000$ simulation
246 runs). For two-photon data, a minuscule, but significant, trend was evident (bootstrapped PCA
247 slope = 0.03 ± 0.1 s.e., $n = 7151$). So while selective inputs are proposed to provide more
248 information about encoded stimulus variables (Seriès et al., 2004; Shamir and Sompolinsky,
249 2006; Zavitz and Price, 2019) and unselective (or poorly selective) inputs could convey
250 information through their covariance with selective neurons (Zylberberg, 2017), our model and

251 experimental data suggest co-tuned and orthogonally-tuned inputs exhibit a wide range of tuning
252 selectivity. Response variability (i.e. standard deviation) across trials for simulated excitatory
253 inputs was significantly smaller for ‘null’ orientations (± 90 deg) than at the ‘preferred’ (median =
254 0.30 and IQR = 0.14, median = 0.38 and IQR = 0.22, respectively; $p < 0.001$, Wilcoxon ranksum
255 test). This trend was also observed in our two-photon data (null: median = 0.13 and IQR = 0.15;
256 preferred: median = 0.23 and IQR = 0.31, respectively; $p < 0.001$, Wilcoxon ranksum test). As
257 both modeled and imaged neurons had “null”-tuned excitatory inputs that exhibited less response
258 variability, these inputs may carry useful information about when the preferred stimulus is *not*
259 present.

260 Taken together, our decoding framework with a realistic (i.e. heterogenous orientation
261 tuning), noisy input populations suggest the collection of orthogonally-tuned excitatory inputs in
262 cortical neurons *in vivo* are not unexpected. Instead, the synaptic architecture of layer 2/3 neurons
263 in ferret visual cortex are likely optimized for the readout of upstream populations tuned to
264 orientation.

265

266 Discussion

267

268 We used a population decoding framework (Jazayeri and Movshon, 2006; Kohn et al.,
269 2016; Pouget et al., 2000; Shamir, 2014) to elucidate a possible source of synaptic diversity in
270 functional response properties. We find that even simple decoders exhibit substantial
271 heterogeneity in their weights when the inputs are noisy, correlated neural populations with
272 heterogeneous orientation tuning. We argue that this could naturally explain the heterogeneity in
273 synaptic inputs measured *in vivo* if these cortical neurons are decoding information from upstream
274 input populations. We compared two neural decoders: one with homogenous input (Jazayeri and
275 Movshon, 2006) and one with heterogenous input (Ecker et al., 2011). We show that empirical
276 measurements from dendritic spines recorded within individual cortical neurons in ferret V1 exhibit
277 a similar amount of diversity in orientation tuning as simulated inputs (i.e. excitatory weights) from
278 heterogeneous input populations. It may appear trivial that heterogeneous input populations
279 would produce heterogeneous weights, but it was neither immediately obvious that the weights
280 would not be smooth nor that excitatory weights would be evident for orthogonal orientations.
281 Orthogonally-tuned or non-preferred inputs are often considered to be aberrant; to be pruned
282 away during experience-dependent plasticity or development (Holtmaat and Svoboda, 2009). Our
283 decoding approach suggests these inputs are purposeful and emerge through development as
284 cortical circuits learn the statistics of their inputs (Avitan and Goodhill, 2018). Taken together, our

285 results shed light on synaptic diversity that has been puzzling, suggesting that it is, in fact,
286 expected given known properties of the input population.

287 We believe our study is a significant step forward in combining population coding theory
288 (Averbeck et al., 2006; Pouget et al., 2000) and functional connectomics (Wilson et al., 2016).
289 The ability to measure receptive field properties and statistics of sensory-driven responses of
290 synapses *in vivo* provides a new testing bed for population codes. The individual neurons which
291 synapses converge on are the real components of what has long been a hypothetical downstream
292 population decoder. While we did not set out to build a computational or biophysical model of a
293 neuron, we believe simplistic approaches such as ours are fruitful for understanding basic
294 principles.

295 To limit complexity, our decoder did not account for many aspects of cortical networks
296 such as stimulus-dependent correlations or recurrent connections. In the case of stimulus
297 dependent covariance, the optimal decoder is no longer linear, however, that decoder closely
298 resembles a complex cell (Jaini and Burge, 2017; Pagan et al., 2016). Extending a decoding
299 framework to include realistic noise has been used to capture many nonlinear features of neural
300 responses including divisive normalization, gain control, and contrast-dependent temporal
301 dynamics— all features which fall naturally out from a normative framework (Chalk et al., 2017).
302 These more sophisticated approaches may be able to make predictions about the synaptic
303 organization itself, whereby local clusters of synapses act as nonlinear subunits (Ujfalussy et al.,
304 2018).

305 Our model does not describe a cortical transformation. Instead, to limit complexity, we
306 focused on the propagation of orientation selectivity from one neural population to another, akin
307 to the propagation of basic receptive field properties from V1 to higher-visual areas. Our approach
308 was chosen to provide a starting point for predicting the tuning diversity of synaptic input
309 populations as compared to the tuning output or downstream cells. However, this model could be
310 modified to study the convergence and transformation of cortical inputs. An obvious case study
311 would be complex cells in layer 2/3 V1 (Hubel and Wiesel, 1962; Movshon et al., 1978; Spitzer
312 and Hochstein, 1988), which are thought to integrate across presynaptic cells with similar oriented
313 receptive field with offset spatial subunits to produce polarity invariance. This extension would be
314 better suited for a nonlinear quadratic decoder (Jaini and Burge, 2017; Pagan et al., 2016), rather
315 than the linear one used here. We hope that future studies build upon this modeling framework,
316 exploring quadratic decoders and work towards using richer visual stimuli and neural models
317 (Chalk et al., 2017). We believe this will be critical for gaining insight into how information

318 propagates between cortical areas and from largescale measurements of cortical functional
319 connectivity.

320 **Materials and Methods**

321

322 All procedures were performed according to NIH guidelines and approved by the
323 Institutional Animal Care and Use Committee at Max Planck Florida Institute for Neuroscience.

324

325 *Derivation for a Bayesian probabilistic decoder*

326

327 We construct a probabilistic decoder, represented by a population of neurons, that reports
328 or estimates the identity of a stimulus from the spiking response of an input population of neurons.
329 We assume an input population with responses that are a function of the stimulus, $f(\theta_k)$, plus
330 Gaussian noise, $f(\theta_k)$, and the covariance (Q) is equal for all stimulus conditions (Q) such that Q
331 $= Q_k = Q_i$. Then, the posterior distribution can be written as

$$332 \quad p(\theta_k|R) = \frac{p(\theta_k) N(f(\theta_k), Q)}{\sum_i^K p(\theta_i) N(f(\theta_i), Q)}$$

333 where a multivariate Gaussian is

$$334 \quad N(f(\theta_k), Q) = 2\pi^{-\frac{n}{2}} |Q|^{-\frac{1}{2}} e^{\left(-\frac{1}{2}(\mathbf{R}-f(\theta_k))^T Q^{-1}(\mathbf{R}-f(\theta_k))\right)}$$

335 This can be expanded and simplified such that

$$336 \quad p(\theta_k|R) = \frac{p(\theta_k) 2\pi^{-\frac{n}{2}} |Q|^{-\frac{1}{2}} e^{\left(-\frac{1}{2}(\mathbf{R}-f(\theta_k))^T Q^{-1}(\mathbf{R}-f(\theta_k))\right)}}{\sum_i^K p(\theta_i) 2\pi^{-\frac{n}{2}} |Q|^{-\frac{1}{2}} e^{\left(-\frac{1}{2}(\mathbf{R}-f(\theta_i))^T Q^{-1}(\mathbf{R}-f(\theta_i))\right)}}$$

$$337 \quad p(\theta_k|R) = \frac{p(\theta_k) e^{\left(-\frac{1}{2}(\mathbf{R}^T Q^{-1} \mathbf{R} - f(\theta_k)^T Q^{-1} \mathbf{R} - \mathbf{R}^T Q^{-1} f(\theta_k) + f(\theta_k)^T Q^{-1} f(\theta_k))\right)}}{\sum_i^K p(\theta_i) e^{\left(-\frac{1}{2}(\mathbf{R}^T Q^{-1} \mathbf{R} - f(\theta_i)^T Q^{-1} \mathbf{R} - \mathbf{R}^T Q^{-1} f(\theta_i) + f(\theta_i)^T Q^{-1} f(\theta_i))\right)}}$$

$$338 \quad p(\theta_k|R) = \frac{p(\theta_k) e^{-\frac{1}{2} \mathbf{R}^T Q^{-1} \mathbf{R}} e^{\left(f(\theta_k)^T Q^{-1} \mathbf{R} - \frac{1}{2} f(\theta_k)^T Q^{-1} f(\theta_k)\right)}}{\sum_i^K p(\theta_i) e^{-\frac{1}{2} \mathbf{R}^T Q^{-1} \mathbf{R}} e^{\left(f(\theta_i)^T Q^{-1} \mathbf{R} - \frac{1}{2} f(\theta_i)^T Q^{-1} f(\theta_i)\right)}}$$

$$339 \quad p(\theta_k|R) = \frac{e^{\left(\mathbf{R}^T Q^{-1} f(\theta_k) - \frac{1}{2} f(\theta_k)^T Q^{-1} f(\theta_k) + \ln p(\theta_k)\right)}}{\sum_i^K e^{\left(\mathbf{R}^T Q^{-1} f(\theta_i) - \frac{1}{2} f(\theta_i)^T Q^{-1} f(\theta_i) + \ln p(\theta_i)\right)}}$$

$$340 \quad p(\theta_k|R) = \frac{e^{(\mathbf{R}^T w_k + \beta_k)}}{\sum_i^K e^{(\mathbf{R}^T w_i + \beta_i)}}$$

341 where

$$342 \quad w_k = Q^{-1} f(\theta_k)$$

$$\beta_k = -\left(\frac{1}{2}\right) f(\theta_k)^T Q^{-1} f(\theta_k) + \ln p(\theta_k)$$

Here, w are the weights over k for each neuron in the decoder population and β is a constant term for each k . Importantly, because we assume Gaussian input, with this formulation, w and β are derived closed form. More generally, w and β can be estimated numerically using multinomial logistic regression and this form remains optimal for any input population statistics within the exponential family (e.g., Poisson noise).

Input population model

To generate input populations (P_{IN}), we simulated N neurons responding to a stimulus characterized by orientation ($\theta_k \in [-\pi/2:\pi/2K:\pi/2]$). The response of each neuron, r_i , depends on a tuning function, $f_i(\theta)$, and an additive noise term, ε_i , describing trial-to-trial variability. Noise is correlated across the population, generated from a multivariate Gaussian distribution with zero mean and covariance C . Orientation tuning functions were defined as:

$$f_i(\theta) = \alpha_i + \beta_i e^{\kappa_i [\cos(\theta - \phi_i)^2 - 1]}$$

Here, α is the baseline firing rate, β scales the tuned response, κ scales the tuning bandwidth, and ϕ is the orientation preference of each neuron. For homogeneous P_{IN} all parameters except ϕ were fixed: $(\alpha, \beta, \kappa) = (0, 5, 4)$. For heterogeneous P_{IN} , we sampled parameters to match measurements from macaque V1 (Ringach et al., 2002) and our ferret V1 data. Tuning bandwidth was generated by converting half-width at $1/\sqrt{2}$ height (γ) values from a lognormal distribution ($\mu = -1, \sigma = 0.6$):

$$\kappa = -\log(\sqrt{2}) / (\cos(\gamma^2) - 1)$$

Limited-range correlations were included so neural noise correlation depends on tuning preference difference (Ecker et al., 2011). A correlation matrix, C , was specified by the difference between preferred orientations of neurons and the maximum pairwise correlation, c_o :

$$A_{ij} = c_o e^{-|\delta(\phi_i - \phi_j)|}$$

where δ is the circular difference and

$$C_{ij} = A_{ij} + (1 - c_o)I$$

where I is the identity matrix of size N . We scaled the correlation matrix by the mean firing rate of each neuron to produce Poisson-like noise (Ecker et al., 2011).

Derived weights for a given P_{IN} were artificially smoothed using the following equation from (Park and Pillow, 2011):

$$S_{ij}^{+e} - \left(\rho_1 + \left(\frac{\delta(\phi_i - \phi_j)}{\rho_2} \right) \right)$$

375

376 Here, S^+ is the pseudoinverse of S , $\delta(\phi_i - \phi_j)$ is the circular difference between preferred
377 orientations of neurons, ρ_1 scales the amplitude of smoothing, and ρ_2 scales functional range of
378 smoothing.

379

380 *Population decoder estimation accuracy*

381

382 Decoding accuracy was calculated with the mean-squared-error of the maximum a
383 posterior probability (MAP) estimate across t simulated trials of each stimulus (k):

$$384 \text{error}(k) = \left(\frac{1}{t} \right) \sum_1^t \text{angle}(e^{i(MAP(w_k) - \theta_k)})^2$$

385 Here, w_k are the weights for a given decoder neuron and θ_k is the true stimulus.

386

387 *Viral Injections*

388

389 Briefly, female ferrets aged P18-23 (Marshall Farms) were anesthetized with isoflurane
390 (delivered in O₂). Atropine was administered and a 1:1 mixture of lidocaine and bupivacaine was
391 administered SQ. Animals were maintained at an internal temperature of 37 degrees Celsius.
392 Under sterile surgical conditions, a small craniotomy (0.8 mm diameter) was made over the visual
393 cortex (7-8mm lateral and 2-3mm anterior to lambda). A mixture of diluted AAV1.hSyn.Cre
394 (1:25000 to 1:50000) and AAV1.Syn.FLEX.GCaMP6s (UPenn) was injected (125 - 202.5 nL)
395 through beveled glass micropipettes (10-15 micron outer diameter) at 600, 400, and 200 microns
396 below the pia. Finally, the craniotomy was filled with sterile agarose (Type IIIa, Sigma-Aldrich)
397 and the incision site was sutured.

398

399 *Cranial Window*

400

401 After 3-5 weeks of expression, ferrets were anesthetized with 50mg/kg ketamine and
402 isoflurane. Atropine and bupivacaine were administered, animals were placed on a feedback-
403 controlled heating pad to maintain an internal temperature of 37 degrees Celsius, and intubated
404 to be artificially respirated. Isoflurane was delivered throughout the surgical procedure to maintain
405 a surgical plane of anesthesia. An intravenous cannula was placed to deliver fluids. Tidal CO₂,

406 external temperature, and internal temperature were continuously monitored. The scalp was
407 retracted and a custom titanium headplate adhered to the skull (Metabond, Parkell). A craniotomy
408 was performed and the dura retracted to reveal the cortex. One piece of custom cover-glass (3mm
409 diameter, 0.7mm thickness, Warner Instruments) adhered using optical adhesive (71, Norland
410 Products) to custom insert was placed onto the brain to dampen biological motion during imaging.
411 A 1:1 mixture of tropicamide ophthalmic solution (Akorn) and phenylephrine hydrochloride
412 ophthalmic solution (Akorn) was applied to both eyes to dilate the pupils and retract the nictating
413 membranes. Contact lenses were inserted to protect the eyes. Upon completion of the surgical
414 procedure, isoflurane was gradually reduced and pancuronium (2 mg/kg/hr) was delivered IV.

415

416 *Visual Stimuli*

417

418 Visual stimuli were generated using Psychopy (Peirce, 2007). The monitor was placed 25
419 cm from the animal. Receptive field locations for each cell were hand mapped and the spatial
420 frequency optimized (range: 0.04 to 0.25 cpd). For each soma and dendritic segment, square-
421 wave drifting gratings were presented at 22.5 degree increments (2 second duration, 1 second
422 ISI, 8-10 trials for each field of view).

423

424 *Two photon imaging*

425

426 Two photon imaging was performed on a Bergamo II microscope (Thorlabs) running
427 Scanimage (Pologruto et al., 2003) (Vidrio Technologies) with 940nm dispersion-compensated
428 excitation provided by an Insight DS+ (Spectraphysics). For spine and axon imaging, power after
429 the objective was limited to < 50 mW. Cells were selected for imaging on the basis of their position
430 relative to large blood vessels, responsiveness to visual stimulation, and lack of prolonged
431 calcium transients resulting from over-expression of GCaMP6s. Images were collected at 30 Hz
432 using bidirectional scanning with 512x512 pixel resolution or with custom ROIs (frame rate range:
433 22 - 50 Hz). Somatic imaging was performed with a resolution of 2.05 - 10.24 pixels/micron.
434 Dendritic spine imaging was performed with a resolution of 6.10 -15.36 pixels/micron.

435

436 *Two Photon Imaging Analysis*

437

438 Imaging data were excluded from analysis if motion along the z-axis was detected.
439 Dendrite images were corrected for in-plane motion via a 2D cross-correlation based approach in

440 MATLAB or using a piecewise non-rigid motion correction algorithm (Pnevmatikakis and
441 Giovannucci, 2017). ROIs (region of interest) were drawn in ImageJ; dendritic ROIs spanned
442 contiguous dendritic segments and spine ROIs were fit with custom software. Mean pixel values
443 for ROIs were computed over the imaging time series and imported into MATLAB (Hiner et al.,
444 2017; Sage et al., 2012). $\Delta F/F_0$ was computed by computing F_0 with time-averaged median or
445 percentile filter (10th percentile). For spine signals, we subtracted a scaled version of the dendritic
446 signal to remove back-propagating action potentials as performed previously (Wilson et al., 2016).
447 $\Delta F/F_0$ traces were synchronized to stimulus triggers sent from Psychopy and collected by Spike2.
448 Spines were included for analysis if the SNR of the preferred response exceeded 2 median
449 absolute deviations above the baseline noise (measured during the blank) and were weakly
450 correlated with the dendritic signal (Spearman's correlation, $r < 0.4$). Some spine traces contained
451 negative events after subtraction, so correlations were computed ignoring negative values. We
452 then normalized each spine's responses so that each spine had equal weight. Preferred
453 orientation for each spine was calculated by fitting responses with a Gaussian tuning curve using
454 `lsqcurvefit` (Matlab). Tuning selectivity was measured as the vector strength index (v) for each
455 neuron's response:

$$456 \quad v_i = \frac{\sqrt{\sum (r_i \cos \theta_k)^2 + \sum (r_i \sin \theta_k)^2}}{\sum r_i}$$

457 Here r is the mean responses over the orientations (θ_k) presented for each spine (i). Note, this
458 same index is used to characterize simulated input selectivity.

459

460 *Analysis*

461

462 To compare input tuning (derived synaptic population or measured dendritic spine
463 population) with output tuning (downstream readout or measured somatic tuning) we computed
464 the Pearson Correlation coefficient (Matlab). This correlation was computed on trial-averaged
465 responses across different orientations. For dendritic spines and soma, measured responses
466 across stimulus presentation trials were averaged. For simulated synaptic populations and
467 corresponding downstream readout neuron, we simulated trials by adding noise to each synaptic
468 tuning curve.

469

470 **Code Availability**

471

472 Matlab code to generate input and readout populations used are provided:

473 <https://github.com/schollben/SpineProbabilisticModel2020>

474 **Figure Legends**

475

476 **Figure 1: A population decoding framework to study synaptic diversity.**

477 An upstream population of neurons are tuned for a single stimulus variable (orientation) (*top*).

478 This input population is readout by downstream decoder neurons (*bottom*). Downstream neurons

479 decode stimulus identify by reading out spikes from the upstream input population. Each decoder

480 neuron is defined by a set weights (*middle*) over the upstream population, which are summed and

481 rectified to produce an output.

482

483 **Figure 2: Model simulations with homogenous and heterogeneous input populations.**

484 (a) Orientation tuning of a homogenous input population. Shown is a subset of the total population

485 ($n = 20/1000$). Ordinate is orientation preference, restricted between -90° and 90° . (b) Derived

486 weights for a single decoder neuron (preferring 0°) reading out the homogenous (*blue*) input

487 population in (a). Weights for homogenous populations smoothly vary over orientation space. (c)

488 Response output of the decoder neuron whose weights are shown in (b). (d-f) Same as in (a-c)

489 for a heterogeneous input population with moderate correlation ($c_o = 0.25$). Note that decoder

490 weights for heterogeneous input populations are not smooth.

491

492 **Figure 3: Decoder performance of heterogeneous input populations depends on** 493 **population size, correlations, and weight diversity.**

494 (a) Example weight distribution for a decoder neuron reading out a heterogeneous input

495 population (*top*). Shown are the effects of progressively smoothing weights. Smooth parameters

496 (see Methods) from top to bottom: $(0,0)$, $(0.1,1)$, $(0.2,2)$, $(1,10)$. Ordinate is orientation preference,

497 restricted between -90° and 90° . (b) Decoder performance (inverse mean-squared-error) plotted

498 for homogenous and heterogeneous input populations of increasing size. Simulations here

499 include no correlations ($c_o = 0$). Shading indicates standard error. (c) Same as in (b) for input

500 populations with moderate correlation ($c_o = 0.25$). (d) Same as in (b) for input populations with

501 stronger correlation ($c_o = 0.50$).

502

503 **Figure 4: Simulation of synaptic populations from decoder neuron weight distributions.** (a)

504 Example weight distribution for a single decoder neuron tuned to 0° (*left*). Ordinates are

505 orientation preference, restricted between -90° and 90° . Dashed line separates excitatory

506 (positive) and inhibitory (negative) weights. Excitatory weight distribution over the input population
507 is transformed into a frequency distribution, whereby greater amplitude equates to greater
508 frequency of occurrence (*right*). (b) Example simulated synaptic population ($n = 100$ spines) from
509 the weight distribution in (a). Shown are the orientation tuning curves of each simulated synapse
510 (normalized).

511
512 **Figure 5: Orientation tuning diversity of dendritic spine populations in ferret V1 match**
513 **simulations with correlated, heterogeneous input populations.**

514 (a) Two-photon standard-deviation projection of example dendrite and spines recorded from a
515 single cell (*left*). Inset: Two-photon standard-deviation projection of corresponding soma. Scale
516 bar is 10 microns. Orientation tuning of soma (*top*) and all visually-responsive dendritic spines
517 from this single cell ($n = 159$) are shown (*right*). Spine responses are normalized peak $\Delta F/F$.
518 Orientation preferences are shown relative to the somatic preference (aligned to 0°). (b) Same as
519 in (a) for another example cell ($n = 162$ visually-responsive spines). (c) Cumulative distributions
520 of tuning correlation between individual dendritic spines or simulated synaptic inputs with
521 corresponding somatic tuning or decoder output. Shown are correlations of simulations of
522 homogenous (*blue*) or heterogeneous (*red*) input populations, compared to empirical data (*gray*).
523 (d) Distributions of average tuning correlation between synaptic input and somatic output across
524 measured cells ($n = 45$). Also shown are distributions of average tuning correlation for simulated
525 cells. Triangles denote median values for each distribution. (e) Comparison of Kullback-Leibler
526 divergence (D_{KL}) between data and each model type. Each data point represents an individual
527 cell's population of dendritic spines.

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529

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