The structural connectome constrains fast brain dynamics

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Abstract

Brain activity during rest displays complex, rapidly evolving patterns in space and time. Structural connections comprising the human connectome are hypothesized to impose constraints on the dynamics of this activity. Here, we use magnetoencephalography (MEG) to quantify the extent to which fast neural dynamics in the human brain are constrained by structural connections inferred from diffusion MRI tractography. We characterize the spatio-temporal unfolding of whole-brain activity at the millisecond scale from source-reconstructed MEG data, estimating the probability that any two brain regions will activate at consecutive time epochs. We find that the structural connectome profoundly shapes rapid spreading of neuronal avalanches, evidenced by a significant association between these transition probabilities and structural connectivity strengths (r=0.30-0.38, p<0.0001). This finding opens new avenues to study the relationship between brain structure and neural dynamics.

Introduction

The structural scaffolding of the human connectome[1] constrains the unfolding of large-scale coordinated neural activity towards a restricted *functional repertoire*[2]. While functional magnetic resonance imaging (fMRI) can elucidate this phenomenon at relatively slow timescales[3–5], brain activity shows rich dynamic behaviour across multiple timescales, with faster activity nested within slower ones. Here, we exploit the high temporal resolution of resting-state magnetoencephalography (MEG) data to study the spatial spread of neuronal avalanches in healthy adults, aiming to establish whether the structural connectome constrains the spread of avalanches among regions[6,7]. We find that avalanche spread is significantly more likely between pairs of grey matter regions that are structurally connected, as inferred from diffusion MRI tractography. This result provides cross-modal empirical evidence suggesting that connectome topology constrains fast-scale transmission of neural information, linking brain structure to brain dynamics.

Results

Structural connectomes were mapped for 58 healthy adults (26 females, mean age ± SD: 30.72 ± 11.58) using diffusion MRI tractography and regions defined based on the Automated Anatomical Labeling (AAL) and the Desikan-Killiany-Tourville (DKT) atlases. Interregional streamline counts derived from whole-brain deterministic tractography quantified the strength of structural connectivity between pairs of regions (see SI extended methods). Group-level connectomes were computed by averaging connectivity matrices across participants.

MEG signals were pre-processed and source reconstructed for both the AAL and DKT atlases. Each source reconstructed signal was z-scored and binarized such that, at any time point, a z-score exceeding a given threshold was set to 1 (active); all other timepoints were set to 0 (inactive). An avalanche was defined as starting when any region exceeded this threshold, and finished when no region was active. An avalanche-specific transition matrix (TM) was calculated, where element (*i*, *j*) represented the probability that region *j* was active at time *t+δ*, given that region *i* was active at time *t*, where *δ*~3ms. The TMs were averaged per participant, and then per group, and finally symmetrized.

We found striking evidence of an association between avalanche transition probabilities and structural connectivity strengths (Figure 2), suggesting that regional propagation of fast-scale neural avalanches is partly shaped by the axonal fibers forming the structural connectome (r=0.30-0.38, p<0.0001). Specifically, the association was evident for different activation thresholds and both the AAL and DKT connectomes (AAL atlas: for threshold z=2.5, r=0.38; for threshold z=3.0, r=0.37; for threshold z=3.2, r=0.34; DKT atlas: for threshold z=2.5, r=0.32; for threshold z=3.0, r=0.31; for threshold z=3.2, r=0.30; in all cases, p <0.0001), as well as for individual- and group-level connectomes, although associations were stronger for group-level analyses (see Figure 2, panel A).

Next, we sought to test whether the associations were weaker for randomized transition matrices computed after randomizing the times of each avalanche while keeping the spatial structure unchanged (see SI extended methods). Randomized transition matrices resulted in markedly weaker associations with structural connectivity, compared to the actual transition matrices (AAL atlas, z-score=3: mean r = 0.25, observed r= 0.38, p<0.001). This suggests that the empirical organization of the connectome significantly shapes the temporally resolved propagation of neural activity. We replicated these findings for a group-level connectome derived using data from 200 healthy adults in the Human Connectome Project (r=0.11, p<0.001, z-score=3; Materials and Methods). Our results were thus robust to multiple connectome mapping pipelines and parcellation atlases, significant for both group-averaged and individual connectomes, and could not be explained by chance transitions.

Discussion

Our results provide new insight into the propagation of fast-evolving brain activity in the human connectome. We show that the spatial unfolding of neural dynamics at the millisecond scale is shaped by the network of large-scale axonal projections comprising the connectome, thereby constraining exploration of the brain's putative functional repertoire. While previous studies provide evidence of coupling between structural connectivity and functional MRI activity [3,8,9], the neural signals measured with MEG in the present study are orders of magnitude faster, enabling investigation of intrinsic neural dynamics nested in slow activity [10]. Our findings suggest that long-term structure-function coupling previously uncovered with functional MRI occurs against a backdrop of faster fluctuations, which are also constrained by the connectome and may enable individuals to rapidly respond to changing environments and new cognitive demands [11]. Finally, our results explain how the large-scale activity unfolding in time might lead to the previous observation that average resting-state functional connectivity has topological features that mirror those of the structural connectome [12]. The neural avalanche framework opens up new opportunities to investigate polysynaptic models of network communication, which aim to describe patterns of signalling between anatomically unconnected regions [13,14]. Therefore, our work provides a foundational step towards elucidating the mechanisms governing communication in the human connectome. In turn, this can be exploited to predict the effects of structural lesions on behaviour and/or clinical phenotypes, under the above-mentioned hypothesis that structure influences behavioural outcomes by constraining global dynamics. In conclusion, using MEG to study neuronal avalanches, we provide a new framework to link fast neural dynamics to the structural connectome.

Materials and Methods

MEG pre-processing

MEG pre-processing and source reconstruction were performed as in [15], using the FieldTrip toolbox. The registration was acquired at 1024 Hz and divided in two eyes-closed segments of 3:30 minutes each. Principal Component Analysis and Independent Component Analysis were used to remove environmental noise and physiological artifacts, respectively; noisy channels were removed manually. 47 subjects were selected for further analysis. The time series of neuronal activity were reconstructed based on the Automated Anatomical Labeling (AAL) and the Desikan-Killiany-Tourreville (DKT) atlases, using the Linearly Constrained Minimum Variance (LCMV) beamformer algorithm and the native MRIs. We excluded the cerebellar ROIs because of their low reliability in MEG (however, including them did not affect the results).

Transition matrices

Each source reconstructed signal was binned (to obtain a branching ratio ~=1, see SI) and then z-scored and binarized, such that, at any time bin, a z-score exceeding 3 was set to 1 (active); all other time bins were set to 0 (inactive) - see SI. Alternative z-score thresholds (i.e. 2.5 and 3.5) were tested. An avalanche was defined as starting when any region is above threshold, and finishing when no region is active, as in [15]). Avalanches shorter than 10 time bins (30 msec) were excluded. However, including only avalanches longer than 30 time bins (90 msec), to focus on rarer events that are highly unlikely to be noise, and including all avalanches, did not affect the results. An avalanche-specific transition matrix (TM) was calculated, where element (i, j) represented the probability that region j was active at time $t+\delta$, given that region i was active at time t, where $\delta \sim 3ms$. The TMs were averaged per participant, and then per group, and finally symmetrized.

Diffusion MRI pre-processing and structural connectome mapping

Diffusion MRI data were acquired using a 1.5 Tesla machine. Data were corrected for head movements and eddy current distortions using the "eddy_correct" routine, rotating diffusion sensitizing gradient directions, and a brain mask was obtained from the B0 images. A diffusion-tensor model was fitted at each voxel, and fiber tracks were generated over the whole brain using deterministic tractography (FACT propagation algorithm, angle threshold 45°, spline-filtered, masking by the FA maps thresholded at 0.2). For tractographic analysis, the ROIs of the AAL atlas and of a MNI space-defined volumetric version of the Desikan-Killiany-Tourville (DKT) ROI atlas were used, both masked by the GM tissue probability map available in SPM (thresholded at 0.2). Individual FA volumes were normalized to the MNI space using the FA template provided by FSL, using the spatial normalization routine available in SPM12, and the resulting normalization matrices were inverted and applied to the ROIs, to apply them onto each individual. The quality of the normalization was assessed visually. For each individual, the number of streamlines interconnecting each pair of regions was enumerated using custom software written in Interactive Data Language. In supplementary analyses, connectomes were also mapped using diffusion MRI data for 200 participants from the Human Connectome Project using an

alternative workflow. The resulting individual connectomes were then averaged to yield a group-consensus connectome (see SI).

Statistical analysis

The Spearman rank correlation coefficient was used to assess the association between transition probabilities and structural connectivity. A correlation coefficient was computed separately for each individual across all pairs of regions. Transition matrices were symmetrized before this computation.

Randomized transition matrices were generated to ensure that associations between transition probabilities and structural connectivity could not be attributed to chance. Avalanches were randomized across time, without changing the order of avalanches at each time step. We generated a total of 1000 randomized transition matrices and the Spearman rank correlation coefficient was computed between each randomized matrix and structural connectivity. This yielded a distribution of correlation coefficients under randomization. The proportion of correlation coefficients that were greater than, or equal to, the observed correlation coefficient provided a p-value for the null hypothesis that structure-function coupling was attributable to random transition events.

References

1. Sporns, O., Tononi, G. & Kötter, R. The Human Connectome: A Structural Description of the Human Brain. *PLoS Comput. Biol.* **1**, e42 (2005).
2. Deco, G., Jirsa, V. K. & McIntosh, A. R. Emerging concepts for the dynamical organization of resting-state activity in the brain. *Nature Reviews Neuroscience* vol. 12 43–56 (2011).
3. Honey, C. J., Kötter, R., Breakspear, M. & Sporns, O. Network structure of cerebral cortex shapes functional connectivity on multiple time scales. *Proc. Natl. Acad. Sci. U. S. A.* **104**, 10240–5 (2007).
4. Goni, J. *et al.* Resting-brain functional connectivity predicted by analytic measures of network communication. *Proc. Natl. Acad. Sci. U. S. A.* **111**, 833–838 (2014).
5. Zalesky, A., Fornito, A., Cocchi, L., Gollo, L. L. & Breakspear, M. Time-resolved resting-state brain networks. *Proc. Natl. Acad. Sci. U. S. A.* **111**, 10341–6 (2014).
6. Beggs, J. M. & Plenz, D. Neuronal Avalanches Are Diverse and Precise Activity Patterns That Are Stable for Many Hours in Cortical Slice Cultures. *J. Neurosci.* **24**, 5216–5229 (2004).
7. Shriki, O. *et al.* Neuronal avalanches in the resting MEG of the human brain. *J. Neurosci.* **33**, 7079–7090 (2013).
8. Honey, C. J., Thivierge, J. P. & Sporns, O. Can structure predict function in the human brain? *NeuroImage* vol. 52 766–776 (2010).
9. Honey, C. J. *et al.* Predicting human resting-state functional connectivity from structural connectivity. *Proc. Natl. Acad. Sci. U. S. A.* **106**, 2035–2040 (2009).
10. Saggio, M. L., Spiegler, A., Bernard, C. & Jirsa, V. K. Fast–Slow Bursters in the Unfolding of a High Codimension Singularity and the Ultra-slow Transitions of Classes. *J. Math. Neurosci.* **7**, 1–47 (2017).
11. Mcintosh, A. & Jirsa, V. The hidden repertoire of brain dynamics and dysfunction. *Netw. Neurosci.* **3**, (2019).
12. Bullmore, E. & Sporns, O. Complex brain networks: graph theoretical analysis of structural and functional systems. *Nat. Rev. Neurosci.* **10**, 186–198 (2009).
13. Seguin, C., Van Den Heuvel, M. P. & Zalesky, A. Navigation of brain networks. *Proc. Natl. Acad. Sci. U. S. A.* **115**, 6297–6302 (2018).
14. Seguin, C., Razi, A. & Zalesky, A. Inferring neural signalling directionality from undirected structural connectomes. *Nat. Commun.* **10**, 1–13 (2019).
15. Sorrentino, P. *et al.* Extensive functional repertoire underpins complex behaviours: insights from Parkinson's disease. *bioRxiv* 823849 (2019) doi:10.1101/823849.

Figure 1. A. Rendering of streamlines reconstructed using diffusion MRI and tractography **B.** Structural connectivity matrix. Row/columns represent regions; matrix entries store the number of streamlines interconnecting each pair of regions. **C.** Source-reconstructed MEG series. Blue lines represent the z-scored regional activity, and the red lines denote the threshold (z-score= ± 3). In the inset: magnified time-series exceeding the threshold. **D.** Avalanche Raster plot. For each region, the moments in time when the activity is above threshold are represented in black, while the other moments in white. The particular avalanche that is represented involved three regions. **E.** Estimation of the transition matrix of a toy avalanche. Region *i* is active three times during the avalanche. In two instances, denoted by the green arrows, region *j* was active after region *i*. In one instance, denoted by the red arrow, region *i* is active but region *j* does not activate at the following time step. This situation would result, in the transition matrix, as a 2/3 probability. **F.** Average structural matrix and average transition matrix (Log scale).

Figure 2. A. Distribution of the r's of the Spearman's correlation between the subject-specific transition matrices and structural connectomes. The black diamond represent the r's of the group-averaged matrices. On the left, the results for the AAL atlas, on the right, the results for the DKT atlas. Green, purple and orange dots represent results obtained with a z-score threshold of 2.5, 3 and 3.5, respectively. **B and C.** Data referring to the AAL atlas in B, to the DKT atlas in C. On the top-left, the average structural matrix, on the bottom left, the average transition matrix. The scatterplot shows the correlation between the values of the structural edges and the transition probabilities for the corresponding edge. The black line represents the best fit line in the least-square sense. On the right, the distribution shows the r's derived from the null distribution. The dotted blue line represents the observed r.