Main Manuscript for

Altered functional integration of brain activity is a marker of impaired cognitive performance following sleep deprivation

Nathan E. Cross[1,2,3], Florence B. Pomares[1,2,3], Alex Nguyen[1,2,4], Aurore A. Perrault[1,2,3], Aude Jegou[1,4], Makoto Uji[1,2,4], Kangjoo Lee[4], Fatemeh Razavipour[1,4,5], Obaï Bin Ka'b Ali[1,4,5], Umit Aydin[1,4,5], Habib Benali[1], Christophe Grova[1,4,5*] and Thien Thanh Dang-Vu[1,2,3*]*

[1] PERFORM Centre, Concordia University, Montreal, Canada

[2] Center for Studies in Behavioral Neurobiology, Department of Health, Kinesiology and Applied Physiology, Concordia University, Montreal, Canada

[3] Institut Universitaire de Gériatrie de Montréal and CRIUGM, CIUSSS du Centre-Sud-de-l'Île-de-Montréal, Montreal, Canada

[4] Multimodal Functional Imaging lab, Department of Physics, Concordia University, Montreal, Canada

[5] Multimodal Functional Imaging Lab, Biomedical Engineering Dpt, Neurology and Neurosurgery Dpt, McGill University, Montreal, Quebec, Canada

* Nathan Cross, Christophe Grova, Thien Thanh Dang-Vu

Email: nathan.cross@concordia.ca; christophe.grova@concordia.ca; tt.dangvu@concordia.ca

Classification

Paste the major and minor classification here. Dual classifications are permitted, but cannot be within the same major classification.

Keywords

sleep, fMRI, integration, cognition,

Author Contributions

Paste the author contributions here.

This PDF file includes:

Main Text (4200 words)
Figures 1 to 4

Abstract

Sleep deprivation leads to impairments in cognitive function. Here, we tested the hypothesis that cognitive changes in the sleep-deprived brain may be explained by information processing within and between large scale cortical networks. We acquired functional magnetic resonance imaging (fMRI) scans of 20 healthy volunteers during attention and executive tasks following a regular night of sleep, a night of sleep deprivation, and a recovery nap. Overall, sleep deprivation is associated with increased cortex-wide integration, driven by greater within network integration. The relative ration of within-between network integration in the sleep deprived state was tightly associated with deficits in cognitive performance. This was a distinct and better predictor of cognitive impairment than subjective and objective markers of homeostatic sleep pressure, as well as the pronounced thalamo-cortical connectivity changes that occurs towards falling asleep. The ratio of within vs between network integration in the cortex increased further in the NREM sleep, suggesting that prolonged wakefulness drives the cortex toward a state resembling sleep. Importantly, reversal of the balance between segregation and integration of cortical activity was related to both performance decline following SD, and recovery after the nap. Leveraging intra- and inter-individual differences in network integration and segregation may play a critical role in identifying vulnerability to cognitive impairment in the sleep deprived state.

Significance Statement

Paste your significance statement here. Please note that it should not exceed 120 words, but should be at least 50 words in length. It should not include any references.

Introduction

The cognitive consequences of acute total sleep deprivation (SD) are substantial, affecting a wide range of mental processes such as attention, vigilance and working memory (Alhola et al. 2007, Killgore 2010). Yet the measurable impact of SD on cognition varies across individuals (Rupp et al. 2012, Dennis et al. 2017). Brain activity patterns have significant potential in revealing inter-individual effects of prolonged wakefulness on cognitive functioning (Patanaik et al. 2018, Yeo et al. 2015).

Level of arousal has a significant influence over endogenous brain activity fluctuations (Podvalny et al. 2019, McGinley et al. 2015). Increased power of slower frequency (0.5-8Hz) brain rhythms during wakefulness is a prominent feature of the sleep deprived state (Oken et al. 2006, Smith et al. 2002). Additionally, the global signal (GS), a reference to the mean fMRI activity measured either across the entire brain or grey matter, fluctuates at a significantly greater magnitude in states of reduced arousal and vigilance (Wong et al. 2013), as well as following SD (Yeo et al. 2015). These endogenous activity fluctuations in the human brain share a robust association with ongoing cognitive and perceptual processes (Podvalny et al. 2019), as they may interfere with the capacity for information processing.

Both localized brain regions and cortical networks display characteristic and independent (segregated) activity patterns whether measured at rest or during the performance of actions (Fox et al. 2012, Di et al. 2013). However, even simple behaviors and cognitive processes require the coordination (integration) of information flows across systems distributed in the brain (Varela et al. 2001). It has been proposed that efficient cognitive functioning is reflected through a balance of segregation and integration of activity across brain networks (Sporns et al. 2004, Tononi et al. 1994). Therefore, in states of reduced arousal, an elevation in widespread slow wave patterns across the cortex may affect the ability to integrate information between and within cortical networks, corresponding to the cognitive deficits experienced during these states. These deficits may also be driven by certain changes in subcortical regions, such as the thalamus, which is involved in both maintaining cortical arousal (Van der Werf et al. 2002) and constraining the engagement of distributed neural assemblies within the cerebral cortex (Shine 2020). However, this has not been explored following experimental manipulation of arousal states, such as SD. Furthermore, SD induced cognitive impairment partially improves with subsequent sleep (Lo et al. 2016). Yet it remains unclear whether this behavioral recovery is associated with a functional 'recovery' of cortical networks after sleep.

Here we assessed principles of functional brain activity across various arousal states using EEG-fMRI and a sleep deprivation protocol. Participants were scanned both at rest and whilst performing cognitive tasks of attention, executive control and working memory, after both a regular night of sleep and 24hrs of SD. Additionally, we measured EEG-fMRI activity during a recovery nap containing NREM sleep, as well as during a post recovery nap (PRN) session when the rest and task sequences were repeated. Firstly, to quantify the functional interactions within and between cortical networks across vigilance states, we computed a measure of integration between and within functional networks across different hierarchical levels of the cortex (Boly et al. 2012, Marrelec et al. 2008). We then compared the changes in functional integration to the magnitude of cognitive impairment following SD. In addition, we measured the association between recovery of both performance and the integration of cortical networks following the nap. Next, we assessed these changes in the context of changes to the amplitude of both local

activity patterns and the global brain signal. Finally, we investigated the influence of thalamocortical activity on functional integration in the cortex across different arousal states.

Results

Twenty participants (mean age of 21.2 ± 2.5 years, 12 females) participated in the study. In each session (Rested Wakefulness, RW; SD; PRN) participants completed a 5-minute resting state sequence (fixation cross). Participants also completed 3 cognitive tasks. Two were focused on attention - the Attention Network Task (ANT (Fan et al. 2002), 13min) and the Mackworth Clock Task (MCT (Lichstein et al. 2000), 5min). The other focused on working memory - the N-back task (Kirchner 1958) (8min). As expected, performance outcomes (accuracy and reaction time) across all tasks were significantly impaired following SD, and improved following the recovery nap (SI Results, Fig. S1).

13 participants had brief sleep episodes (<10s) and 4 fell asleep (>30s) during the resting state sequences in the SD condition. In addition to excessive head motion (average framewise displacement: 0.18 ± 0.09mm vs 0.24 ± 0.14mm during RW), this resulted in these sequences not being used in the main analyses, however results from the resting state data can be found in SI Results (Fig S3). None of the subjects in the final sample fell asleep during the cognitive tasks. Additionally, head movement inside the scanner during the cognitive tasks was not significantly different between the sessions (average framewise displacement: 0.17 ± 0.11mm (RW) vs 0.20 ± 0.12mm (SD); $F = 2.36$, $p = 0.109$).

The fMRI data across the multiple tasks were concatenated temporally for every subject, resulting in a 26min long timeseries of blood oxygen level dependent (BOLD) signal (Fig. S2). The general task-specific activity (i.e. for all trials for the ANT and all blocks for the MCT and N-back tasks) was regressed out from the BOLD timeseries as has been implemented in previous studies (De Havas et al. 2012, Wang et al. 2016) to reduce the influence of task-evoked activations in connectivity and integration analyses. The BOLD data sampled along the cortical surface was clustered into 400 parcels (Schaefer et al. 2018), which were further categorised into 7 networks, 17 networks (Yeo et al. 2011), and 57 clusters in a hierarchical fashion (Fig. S2). Integration of activity at each level of this hierarchical structure was computed from the covariance matrix of the cortical parcels activity over time and compared between states within a Bayesian framework (Boly et al. 2012, Marrelec et al. 2008).

Altered Functional Integration in the Cerebral Cortex is Related to Changes in Cognitive Performance

Overall, there was a widespread increase in correlation values (functional connectivity) between cortical parcels from RW to SD (41% of edges, **Fig. 1*A***). This coincided with an increase in the total integration measured across the entire cortex. **Fig. 1*B*** illustrates the changes in functional integration across distinct levels in the hierarchical model of the cortex. At the level of 7 cortical networks, there was an increase in total integration within 4 of the 7 networks: the Dorsal Attention, Limbic, Somatomotor and Visual networks (Table S2). At the 17-network level, both Dorsal Attention (A&B) networks and both Somatomotor (A&B) networks demonstrated increased integration, while only one of the Limbic (B) and Visual (B) networks showed an increase (Table S3). Additionally, there was also increased integration within the Temporal Parietal network. This pattern of change indicates that while the increases in total integration were detectable when measured across the entire cortex, this was not uniform and preferentially affected certain networks and regions (**Fig. 1*C***).

Further deconstructing these changes in integration following SD, we additionally calculated the degree of functional clustering within the cortex. Functional clustering estimates how integration is hierarchically organized within and between the constituent parts of a system, such as networks in the cortex. Specifically, the functional clustering ratio (FCR) is the ratio of within-network integration to between-network integration. There was a significant increase in the FCR at both the level of the entire cortex, and within each of the 7 cortical networks (Table S4). The increase in both total integration and FCR were highly correlated across subjects ($r=0.92$, $p<0.001$). This indicates that the increase in integration observed following SD was significantly more prominent within each network than any increased integration between networks (Figure S4). After parsing each of the 17 networks into assemblies (clusters) based upon a data-driven partition of each network (Fig. S5), the only significant increases in the FCR were observable within the Somatomotor (B), Ventral Attention (A), Default Mode (B), and the Temporal Parietal networks (Table S5).

To assess how the changes in brain activity patterns related to changes in cognitive performance, we first assessed a combination of performance across all tasks. The change (SD-RW) in performance outcomes on each of the 3 separate cognitive tasks were grouped into either accuracy (% of correct responses) or speed (reaction time, ms). The change scores for accuracy or speed were entered into separate Principal Component Analyses (PCA), to obtain resulting principal components that explained the most variance in Accuracy or Speed across the 3 tasks. The first component for Accuracy (explaining 71% of the variance across tasks) was robustly and significantly negatively associated with the change in FCR within the cortex (**Fig. 2*A***). The first component for Speed (explaining 95% of the variance) was also significantly positively correlated with the change in FCR within the cortex. Very similar results were observed for associations between the increase in total integration and performance (SI Results, Fig. S6). The change in integration within each of the 7 networks was negatively correlated with change in Accuracy and Speed from WR to SD (SI Results). We also assessed the change in performance on each task separately in comparison to the change in FCR of cortical BOLD activity during that task only. A greater increase in total integration was significantly related to worse accuracy and speed in the ANT and Nback tasks, but not the MCT (Fig. S7). Finally, a decrease in connectivity was observed from the SD to the PRN state, although to a lesser extent than the increase observed between RW and SD (16.7% of connections, Fig. S8). There was no significant decrease in FCR across the entire cortex (**Fig. 2*B***), and this was not correlated with the duration of the nap or the amount of slow wave sleep (SI Results). However, the subjects who had the greatest decrease in FCR from SD to the PRN, showed the largest improvement in performance for both the Accuracy and Speed outcomes (**Fig. 2*A***). This recovery effect demonstrates a clear link between changes in functional integration and changes in cognitive performance due to SD.

Functional Clustering of Brain Activity Predicts the Conscious State

Following the SD condition, 19 of the 20 participants managed to successfully sleep inside the scanner, for an average of 50 ± 12 minutes (a full sleep summary can be found in Table S6). A stable period of 26 minutes (i.e. the same length as the concatenated task timeseries) consisting of NREM sleep (Stages N2 and N3) was selected from the fMRI scan sequence, and the same connectivity and integration metrics were calculated. During this recovery nap of NREM sleep, the amount of total integration within the cortex was comparable to the RW state, and significantly lower than in the SD state (**Fig. 2*C***). However, the FCR was significantly greater

during NREM sleep than the wake states, for all subjects (**Fig. 2*D***). This was driven by both an increase in within-systems integration as well as a decrease in the integration between-networks (SI Results). These changes demonstrate that the altered balance of within-networks and between-networks integration is a characteristic feature of online vs offline brain states.

Functional Integration is Linked to the Amplitude of Local and Global Signal Fluctuations

We investigated whether the increase in functional integration may be due to regional changes in the amplitude of brain activity fluctuations. Between the RW and SD states, the parcel-wise change in signal fluctuation amplitude (standard deviation) was greatest over the somatosensory cortex and peripheral visual cortex (**Fig. 3*A***). The spatial correspondence between these changes in signal fluctuation and changes in integration at the group level were all significantly correlated, and the relationship was strongest for integration changes at the cluster (assembly) level (**Fig. 3*B***). However, across individuals these changes in signal fluctuation amplitude were mostly only correlated with integration changes in the visual cortex (**Fig. 3*C***).

In line with previous reports, the amplitude of the global signal fluctuation significantly increased from the RW to the SD state (**Fig. 3*D***). In each state, the total functional integration across the cortex significantly correlated with the global signal fluctuation, however the relationship was the strongest during the SD state (**Fig. 3*E***). This suggests that the global signal is strongly associated with measures of functional integration, but these measures become more tightly coupled in periods of reduced arousal, such as following SD. At the WR state, the timeseries of each parcel were only moderately associated with the global signal timeseries, however this increased significantly across a widespread number of parcels, including somatomotor, visual, temporal and parietal regions of the cortex (**Fig. 3*F***) during the SD state, and persisted in the PRN state.

Relationships with Sleepiness and Physiological Markers of Sleep Pressure

Given the increase in both total integration and the FCR within the cortex following SD, we tested whether these were related to the level of homeostatic sleep pressure. Firstly, the change in integration was not associated with subjective sleepiness (Karolinska Sleepiness Score (Shahid et al. 2011)). Neither did the magnitude of the increase in integration or FCR following SD correlate with sleep latency, latency to Stage 3 NREM sleep or the amount of slow wave activity (SWA) during the nap (SI Results). These have all have been previously been shown to be markers of homeostatic sleep pressure, suggesting that functional integration in the cortex is not merely a marker of enhanced sleep pressure.

Changes in Subcortical Connectivity

We also measured subcortical-cortical connectivity to investigate whether these interactions may influence changes in cortical integration in periods of reduced arousal. Out of 6 subcortical regions, there was a notable significant decrease in the correlations between the thalamus and widespread cortical regions following SD (**Fig. 4*A***). Connectivity changes in the thalamus were greatest with the Somatomotor, Dorsal Attention and Temporal Parietal networks (**Fig. 4*B***). However, no correlations between the change in thalamocortical connectivity and cortical integration were observed across individuals (**Fig. 4*C***). Neither were there any relationships observed between thalamocortical connectivity and cognitive performance, or markers of sleep pressure (SI Results). Nevertheless, thalamocortical connectivity was lowest during the SD state, even less than during NREM sleep (**Fig. 4*D***). This was particularly accentuated in the resting

state sequence following SD, a period of sleep-wake instability when the majority of subjects had sleep intrusions (**Fig. 4*D***).

Discussion

These findings demonstrate that the integration within cortical networks increases relative to integration between networks in states of decreasing arousal. The balance of these two integration terms, i.e. the functional clustering ratio (FCR), can be viewed as the degree of functional segregation of a system into its constituent parts (Boly et al. 2012, Tononi et al. 1994). In other words, this signifies how much information the networks of the cortex generate independently, compared with the information generated by the cortex as a whole. The FCR was found to increase across the cortex, and preferentially within certain functional networks (each divided in turn into smaller networks), suggesting that these modifications in information integration were present when measured across different hierarchical levels of the cortex. We detected the greatest FCR during the recovery nap, consistent with previous observations during NREM sleep (Boly et al. 2012). This was driven by both an increase in within-network integration as well as a significant decrease in between-network integration. It is widely accepted that sleep is not merely a state of quiescence, but an active brain state of self-organised, endogenous activity mostly cut-off from the outside world. The level of consciousness has been hypothesised to be related to the degree of integrated information in the brain: that is, the information generated by the interactions in a whole system, above the information generated by the parts (Tononi 2004, Tononi 2008). This is consistent with our observations of integrated brain activity during the recovery nap. Alternatively, in the SD state, the integration between-networks remained stable, which is coherent with the fact subjects remained in a conscious, wakeful state. However, given the increase of within-network integration, the FCR was still significantly higher compared to RW. In summary, following prolonged wakefulness the proportional integration and segregation of brain activity appears to be driven from levels in well-rested wakefulness toward those observed during offline states, such as NREM sleep.

We have recently shown that the primary axes of differentiation in functional connectivity (i.e. functional gradients) across the cortex do not undergo major changes following SD (Cross et al. 2020). This is consistent with the current findings, as although within-network integration increased, between-network functional connectivity remained stable. Furthermore, the gradient approach is sensitive to the shape of the functional connectivity distributions rather than variations in amplitude. Indeed, in this study we found that changes in the integration of brain activity are related to elevated amplitude of brain signal fluctuations, particularly the global signal. The reason behind an increase in signal amplitude during SD is not clear. However, one emerging candidate for a primary role of sleep is the flushing of metabolic waste through the mixing of cerebrospinal and interstitial fluid via the glymphatic system (Iliff et al. 2012, Xie et al. 2013). Large oscillations of fluid inflow into the perivascular space occur during sleep and are tightly coupled with large amplitude slow waves (Fultz et al. 2019, Hablitz et al. 2019). Thus, a build-up of waste products from extended periods of cellular activity in the brain may trigger the mechanisms (i.e. large amplitude slow waves) for the glymphatic system to begin clearing waste, even in the wake state (Xie et al, 2013). Additionally, it is also plausible that a change in respiration or cardiac activity due to parasympathetic drive could account for changes in BOLD activity amplitude, as the greatest changes in integration were detected nearest the middle cerebral artery (Gibo et al. 1981).

Our results demonstrate that disruption to the balance between integration and segregation of cortical networks has a significant impact on effective and efficient cognitive performance. This effect was bidirectional, as both increased FCR following SD negatively correlated with performance, while the decrease in FCR following a recovery nap was associated with the greatest cognitive improvement. Maintaining a balance between integration and segregation of information flow is thought to be crucial for distributed brain networks to execute effective cognitive function (Fox et al. 2012, Tononi et al. 1994). In particular, the ability to dynamically fluctuate between integrated and segregated brain states may be the mechanisms of ongoing cognitive processes (Shine et al. 2016, Sporns 2013). Information generated by the brain would theoretically decrease if dynamic states become more homogenous (indicated by an increase in total integration or global signal amplitude). If the repertoire of dynamic brain states decreases (i.e. many states precede fewer alternatives), then there is less uncertainty in the system and less information is generated (Tononi 2008, Tononi et al. 1994).

We also replicated previous findings demonstrating that SD results in disruptive changes of thalamocortical functional connectivity, including the introduction of negative correlations (Shao et al. 2013, Yeo et al. 2015). The underlying mechanisms and physiological meaning of negative functional connectivity are still unclear (Chen et al. 2011, Fox et al. 2005, Murphy et al. 2009). However, the disruption of thalamocortical connectivity would have a significant impact on the maintenance of cortical arousal. The intralaminar and midline nuclei of the thalamus, with strong inputs from brainstem nuclei, are considered as part of the ascending reticular activating system which stimulate the cortex and facilitate the generation of intrinsic functional modes (Edlow et al. 2012, Kinomura et al. 1996, Van der Werf et al. 2002). The thalamus also serves as the major hub for gating the flow of information into the cerebral cortex by blocking incoming signals through synaptic inhibition of thalamocortical relays. This is proposed to be the main mechanism contributing to shifting the brain from an aroused state into an 'offline' state such as sleep (Steriade et al. 1993).

However, we observed no relationship between the change in thalamocortical connectivity and cortical integration or cognitive performance across subjects (**Fig. 4*C***). Specifically, almost every subject expressed decreased (or anti-correlated) thalamocortical connectivity in the SD state, while there were more varied changes in integration between the RW and SD states across subjects (some not exhibiting relative increases in integration or FCR after 24 hours of SD). There are two possible explanations for these findings. Firstly, during prolonged wakefulness thalamocortical disconnection may precede changes in cortical integration, the latter occurring after different durations of SD across individuals. This is supported by evidence that during sleep onset, thalamic deactivation (i.e. thalamic activity decreasing to overall sleep levels) precedes cortical changes by several minutes (Magnin et al. 2010). This would also be consistent with the observation that the thalamocortical connectivity was at its lowest in the SD resting-state sequence (**Fig. 4*D***), when it was confirmed through EEG that the majority of subjects experienced brief entry into sleep. The alternative possibility is that disrupted thalamocortical connectivity is a state-based effect of SD, while altered cortical integration underlies inter-individual differences in cognitive performance (or cortical 'reserves') following SD. To compare these hypotheses would require repeated measurements of brain activity across an extended period of prolonged wakefulness. Regardless, these results further elucidate the relationship between the thalamus and cortex, demonstrating that in some individuals the cortex can still maintain an optimal balance of integration and segregation required for cognitive processing

despite becoming functionally disconnected from the thalamus. As has been proposed, the ascending modulatory transmitter systems mostly provide the necessary arousal to tune the state and excitability of the different parts of the cortex, which allow for the appropriate analysis of sensory information (i.e. cognitive processing and behavioral responses; (Steriade et al. 1993). Therefore, thalamocortical disruption following SD may not directly cause impaired cognition, but rather be a precipitating factor via altered functional integration in the cortex.

Conclusion

In conclusion, sleep deprivation appears to impact the balance of integration and segregation of brain activity. It is not clear from these findings alone whether these changes are completely neurogenic, or arise from systemic processes involved in maintaining homeostasis of the cellular environment in the brain. Regardless, the disruption of information integration in the brain is significantly linked to the level of cognitive impairment in individuals. Future perspectives should focus on why integration and segregation of brain activity is impaired following sleep deprivation, and how the dynamics of integrated network states are affected during cognitive task performance.

Materials and Methods

Population and Experimental Design. Participants were recruited using advertisements posted online and within Concordia University, Montreal. All participants were 18-30 years old, healthy, regular sleepers and none were taking any medication. Participants made three visits to the sleep laboratory, including a night for habituation + screening to rule out sleep disorders, normal night (8hr sleep, RW) and experimental night (0hr sleep, SD). Each morning in the RW and SD conditions, participants completed three cognitive tasks and one resting state sequence. In the SD condition, participants were provided a 60-min opportunity to sleep inside the MRI, and the tasks and then the resting state sequence were repeated (SI Materials and Methods).

fMRI Data Acquisition and Analysis. MRI scanning was acquired with a 3T GE scanner (General Electric Medical Systems, Wisconsin, US) using an 8-channel head coil. Structural T_1-weighted images with a 3D BRAVO sequence, and functional echo planar images were acquired. Data were preprocessed using the fMRIPrep (Esteban et al. 2019) and xcpEngine (Ciric et al. 2017) toolboxes. The preprocessed BOLD time series for each subject was projected onto the cortical surface and smoothed along the surface using a 6mm smoothing kernel. For each subject and session, the general HRF task-specific activity was regressed out from the BOLD timeseries, and the timeseries from all tasks were concatenated. ***Network and assembly identification.*** The preprocessed BOLD timeseries was then assigned to one of 400 cortical parcels from a standardized parcellation template (Schaefer et al. 2018), where each parcel is also assigned to one of 7 or 17 functional resting state networks (Yeo et al. 2011). Each of the 17 functional networks were further partitioned into assemblies (clusters) based upon a hierarchical clustering that maximized intraclass similarity (SI Materials and Methods). ***Functional connectivity and integration.*** The mean time course of each parcel was correlated to the mean time courses of all other parcels and the correlation values were z-scored. Significance was corrected at $p<0.05$ using the false discovery rate method (Benjamini et al. 1995). Integration was defined as the Kullback–Leibler information divergence between the joint distribution $p(y_1, \dots y_K)$ and the

product of the marginal distributions of the N-dimensional fMRI BOLD time series y divided into K subsets (Marrelec et al. 2008). Integration was calculated at different levels in a hierarchical model of the cortex: whole cortex divided into 7 networks; each of 7 networks divided into small sub-networks (Yeo 17 networks), and; 17 sub-networks divided into 57 clusters (assemblies). We defined the FCR as the ratio between the integration within subsystems (I_{ws}), compared with the integration present between these subsystems (I_{bs}) (SI Materials and Methods).

EEG Data Acquisition and Analysis. EEG was acquired using an MR compatible 256 high-density geodesic sensor EEG array (Electrical Geodesics Inc, *EGI)*. EEG data were recorded using a battery-powered MR-compatible 256-channel amplifier referenced to Cz. Electrocardiography (ECG) was also collected via two MR compatible electrodes through a bipolar amplifier (Physiobox, EGI). The EEG data were corrected for MR gradient ballistocardiographic pulse-related artefacts using the Brainvision Analyzer (*Brain Products Inc, Gilching Germany*). The MR-denoised EEG signal was bandpass filtered between 1 and 20 Hz to remove low-frequency drift and high-frequency noise, down-sampled to 250 Hz, and re-referenced to the linked mastoids. Scoring of the sleep session was performed in conjunction by two trained scorers (NEC, AAP) using the Wonambi toolbox (https://github.com/wonambi-python/wonambi) (using the channels Fz, F3, F4, C3, C4, O1 and O2) in order to obtain measures of sleep including total sleep time, and the duration of sleep stages.

Bayesian Estimation and Statistical Analysis. Probable values of integration and FCR were inferred from the data using a repeated measures approach and Bayesian numerical sampling scheme (1,000 samples per estimate). Using this sampling procedure, the covariance matrices estimated for each individual at each time point were compared to obtain a t-statistic per subject. A second-level one-sample t-test was then performed on these values to infer a significant group difference across time. This approach is similar to that used in estimation of functional activations in fMRI task based paradigms.

Acknowledgments

Paste your acknowledgments here.

References

Alhola, P. and P. Polo-Kantola Sleep deprivation: Impact on cognitive performance. Neuropsychiatric disease and treatment. 2007; **3**(5): 553-567.

Benjamini, Y. and Y. Hochberg Controlling the False Discovery Rate: A Practical and Powerful Approach to Multiple Testing. Journal of the Royal Statistical Society. Series B (Methodological). 1995; **57**(1): 289-300.

Boly, M., V. Perlbarg, G. Marrelec, M. Schabus, S. Laureys, J. Doyon, M. Pélégrini-Issac, P. Maquet and H. Benali Hierarchical clustering of brain activity during human nonrapid eye movement sleep. Proceedings of the National Academy of Sciences of the United States of America. 2012; **109**(15): 5856-5861.

Chen, G., G. Chen, C. Xie and S.-J. Li Negative functional connectivity and its dependence on the shortest path length of positive network in the resting-state human brain. Brain connectivity. 2011; **1**(3): 195-206.

Ciric, R., D. H. Wolf, J. D. Power, D. R. Roalf, G. L. Baum, K. Ruparel, R. T. Shinohara, M. A. Elliott, S. B. Eickhoff, C. Davatzikos, R. C. Gur, R. E. Gur, D. S. Bassett and T. D. Satterthwaite Benchmarking of participant-level confound regression strategies for the control of motion artifact in studies of functional connectivity. Neuroimage. 2017; **154**: 174-187.

De Havas, J. A., S. Parimal, C. S. Soon and M. W. L. Chee Sleep deprivation reduces default mode network connectivity and anti-correlation during rest and task performance. NeuroImage. 2012; **59**: 1745-1751.

Dennis, L. E., R. J. Wohl, L. A. Selame and N. Goel Healthy Adults Display Long-Term Trait-Like Neurobehavioral Resilience and Vulnerability to Sleep Loss. Scientific Reports. 2017; **7**: 18-21.

Di, X., S. Gohel, E. Kim and B. Biswal Task vs. rest—different network configurations between the coactivation and the resting-state brain networks. Frontiers in Human Neuroscience. 2013; **7**(493).

Edlow, B. L., E. Takahashi, O. Wu, T. Benner, G. Dai, L. Bu, P. E. Grant, D. M. Greer, S. M. Greenberg, H. C. Kinney and R. D. Folkerth Neuroanatomic connectivity of the human ascending arousal system critical to consciousness and its disorders. Journal of neuropathology and experimental neurology. 2012; **71**(6): 531-546.

Esteban, O., C. J. Markiewicz, R. W. Blair, C. A. Moodie, A. I. Isik, A. Erramuzpe, J. D. Kent, M. Goncalves, E. DuPre, M. Snyder, H. Oya, S. S. Ghosh, J. Wright, J. Durnez, R. A. Poldrack and K. J. Gorgolewski fMRIPrep: a robust preprocessing pipeline for functional MRI. Nat Methods. 2019; **16**(1): 111-116.

Fan, J., B. D. McCandliss, T. Sommer, A. Raz and M. I. Posner Testing the efficiency and independence of attentional networks. J Cogn Neurosci. 2002; **14**(3): 340-347.

Fox, M. D., A. Z. Snyder, J. L. Vincent, M. Corbetta, D. C. Van Essen and M. E. Raichle The human brain is intrinsically organized into dynamic, anticorrelated functional networks. Proceedings of the National Academy of Sciences of the United States of America. 2005; **102**(27): 9673.

Fox, P. T. and K. J. Friston Distributed processing; distributed functions? NeuroImage. 2012; **61**(2): 407-426.

Fultz, N. E., G. Bonmassar, K. Setsompop, R. A. Stickgold, B. R. Rosen, J. R. Polimeni and L. D. Lewis Coupled electrophysiological, hemodynamic, and cerebrospinal fluid oscillations in human sleep. Science. 2019; **366**(6465): 628.

Gibo, H., C. C. Carver, A. L. Rhoton, Jr., C. Lenkey and R. J. Mitchell Microsurgical anatomy of the middle cerebral artery. J Neurosurg. 1981; **54**(2): 151-169.

Hablitz, L. M., H. S. Vinitsky, Q. Sun, F. F. Stæger, B. Sigurdsson, K. N. Mortensen, T. O. Lilius and M. Nedergaard Increased glymphatic influx is correlated with high EEG delta power and low heart rate in mice under anesthesia. Science Advances. 2019; **5**(2): eaav5447.
Iliff, J. J., M. Wang, Y. Liao, B. A. Plogg, W. Peng, G. A. Gundersen, H. Benveniste, G. E. Vates, R. Deane, S. A. Goldman, E. A. Nagelhus and M. Nedergaard A Paravascular Pathway Facilitates CSF Flow Through the Brain Parenchyma and the Clearance of Interstitial Solutes, Including Amyloid β. Science Translational Medicine. 2012; **4**(147): 147ra111.
Killgore, W. D. S. Effects of sleep deprivation on cognition. Progress in Brain Research. 2010 G. A. Kerkhof and H. P. A. v. Dongen, Elsevier. **185:** 105-129.
Kinomura, S., J. Larsson, B. Gulyás and P. E. Roland Activation by Attention of the Human Reticular Formation and Thalamic Intralaminar Nuclei. Science. 1996; **271**(5248): 512.
Kirchner, W. K. Age differences in short-term retention of rapidly changing information. J Exp Psychol. 1958; **55**(4): 352-358.
Lichstein, K. L., B. W. Riedel and S. L. Richman The Mackworth Clock Test: a computerized version. J Psychol. 2000; **134**(2): 153-161.
Lo, J. C., J. L. Ong, R. L. Leong, J. J. Gooley and M. W. Chee Cognitive Performance, Sleepiness, and Mood in Partially Sleep Deprived Adolescents: The Need for Sleep Study. Sleep. 2016; **39**(3): 687-698.
Magnin, M., M. Rey, H. Bastuji, P. Guillemant, F. Mauguière and L. Garcia-Larrea Thalamic deactivation at sleep onset precedes that of the cerebral cortex in humans. Proceedings of the National Academy of Sciences of the United States of America. 2010; **107**(8): 3829-3833.
Marrelec, G., P. Bellec, A. Krainik, H. Duffau, M. Pélégrini-Issac, S. Lehéricy, H. Benali and J. Doyon Regions, systems, and the brain: hierarchical measures of functional integration in fMRI. Med Image Anal. 2008; **12**(4): 484-496.
McGinley, M. J., M. Vinck, J. Reimer, R. Batista-Brito, E. Zagha, C. R. Cadwell, A. S. Tolias, J. A. Cardin and D. A. McCormick Waking State: Rapid Variations Modulate Neural and Behavioral Responses. Neuron. 2015; **87**(6): 1143-1161.
Murphy, K., R. M. Birn, D. A. Handwerker, T. B. Jones and P. A. Bandettini The impact of global signal regression on resting state correlations: are anti-correlated networks introduced? Neuroimage. 2009; **44**(3): 893-905.
Oken, B. S., M. C. Salinsky and S. M. Elsas Vigilance, alertness, or sustained attention: physiological basis and measurement. Clin Neurophysiol. 2006; **117**(9): 1885-1901.
Patanaik, A., J. Tandi, J. L. Ong, C. Wang, J. Zhou and M. W. L. Chee Dynamic functional connectivity and its behavioral correlates beyond vigilance. NeuroImage. 2018; **177**: 1-10.
Podvalny, E., M. W. Flounders, L. E. King, T. Holroyd and B. J. He A dual role of prestimulus spontaneous neural activity in visual object recognition. Nat Commun. 2019; **10**(1): 3910.
Rupp, T. L., N. J. Wesensten and T. J. Balkin Trait-Like Vulnerability to Total and Partial Sleep Loss. Sleep. 2012; **35**(8): 1163-1172.
Schaefer, A., R. Kong, E. M. Gordon, T. O. Laumann, X. N. Zuo, A. J. Holmes, S. B. Eickhoff and B. T. T. Yeo Local-Global Parcellation of the Human Cerebral Cortex from Intrinsic Functional Connectivity MRI. Cereb Cortex. 2018; **28**(9): 3095-3114.
Shahid, A., K. Wilkinson, S. Marcu and C. M. Shapiro. Karolinska sleepiness scale (KSS). STOP, THAT and One Hundred Other Sleep Scales. 2011, Springer**:** 209-210.
Shao, Y., L. Wang, E. Ye, X. Jin, W. Ni, Y. Yang, B. Wen, D. Hu and Z. Yang Decreased thalamocortical functional connectivity after 36 hours of total sleep deprivation: evidence from resting state FMRI. PLoS One. 2013; **8**(10): e78830.

Shine, J. M. The thalamus integrates the macrosystems of the brain to facilitate complex, adaptive brain network dynamics. Prog Neurobiol. 2020: 101951.
Shine, James M., Patrick G. Bissett, Peter T. Bell, O. Koyejo, Joshua H. Balsters, Krzysztof J. Gorgolewski, Craig A. Moodie and Russell A. Poldrack The Dynamics of Functional Brain Networks: Integrated Network States during Cognitive Task Performance. Neuron. 2016; **92**(2): 544-554.
Smith, M. E., L. K. McEvoy and A. Gevins The impact of moderate sleep loss on neurophysiologic signals during working-memory task performance. Sleep. 2002; **25**(7): 784-794.
Sporns, O. Network attributes for segregation and integration in the human brain. Current Opinion in Neurobiology. 2013; **23**(2): 162-171.
Sporns, O., D. R. Chialvo, M. Kaiser and C. C. Hilgetag Organization, development and function of complex brain networks. Trends in Cognitive Sciences. 2004; **8**(9): 418-425.
Steriade, M., D. A. McCormick and T. J. Sejnowski Thalamocortical oscillations in the sleeping and aroused brain. Science. 1993; **262**(5134): 679.
Tononi, G. An information integration theory of consciousness. BMC Neuroscience. 2004; **5**(1): 42.
Tononi, G. Consciousness as Integrated Information: a Provisional Manifesto. The Biological Bulletin. 2008; **215**(3): 216-242.
Tononi, G., O. Sporns and G. M. Edelman A measure for brain complexity: relating functional segregation and integration in the nervous system. Proceedings of the National Academy of Sciences of the United States of America. 1994; **91**(11): 5033-5037.
Van der Werf, Y. D., M. P. Witter and H. J. Groenewegen The intralaminar and midline nuclei of the thalamus. Anatomical and functional evidence for participation in processes of arousal and awareness. Brain Research Reviews. 2002; **39**(2): 107-140.
Varela, F., J.-P. Lachaux, E. Rodriguez and J. Martinerie The brainweb: Phase synchronization and large-scale integration. Nature Reviews Neuroscience. 2001; **2**(4): 229-239.
Wang, C., J. L. Ong, A. Patanaik, J. Zhou and M. W. Chee Spontaneous eyelid closures link vigilance fluctuation with fMRI dynamic connectivity states. Proc Natl Acad Sci U S A. 2016; **113**(34): 9653-9658.
Wong, C. W., V. Olafsson, O. Tal and T. T. Liu The amplitude of the resting-state fMRI global signal is related to EEG vigilance measures. NeuroImage. 2013; **83**: 983-990.
Xie, L., H. Kang, Q. Xu, M. J. Chen, Y. Liao, M. Thiyagarajan, J. O'Donnell, D. J. Christensen, C. Nicholson, J. J. Iliff, T. Takano, R. Deane and M. Nedergaard Sleep drives metabolite clearance from the adult brain. Science (New York, N.Y.). 2013; **342**(6156): 373-377.
Yeo, B. T., F. M. Krienen, J. Sepulcre, M. R. Sabuncu, D. Lashkari, M. Hollinshead, J. L. Roffman, J. W. Smoller, L. Zollei, J. R. Polimeni, B. Fischl, H. Liu and R. L. Buckner The organization of the human cerebral cortex estimated by intrinsic functional connectivity. J Neurophysiol. 2011; **106**(3): 1125-1165.
Yeo, B. T. T., J. Tandi and M. W. L. Chee Functional connectivity during rested wakefulness predicts vulnerability to sleep deprivation. NeuroImage. 2015; **111**: 147-158.

Figures and Tables

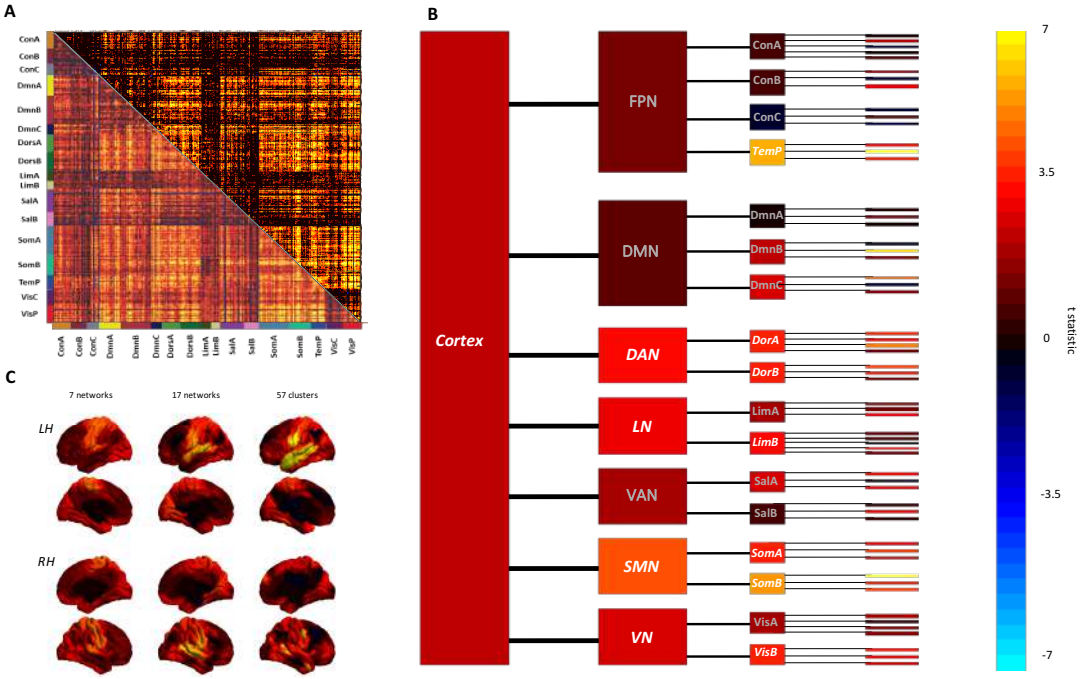
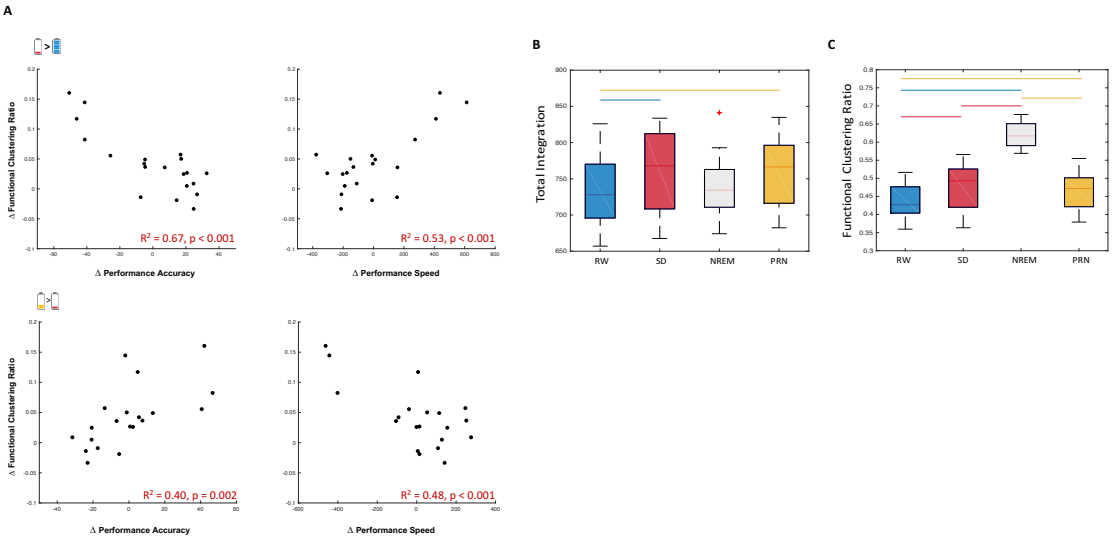


Fig 1. (A) The matrix of change in functional correlations between the timeseries of 400 cortical parcels (during tasks) depicts a widespread increase in correlations between sleep deprivation (SD) and well rested (WR) states (unthresholded, lower triangle; thresholded $P_{FDR}<0.05$, upper triangle). **(B)** Changes in integration are shown across different levels of a hierarchical model of the cortex: whole cortex, 7 networks, 17 networks, and 57 clusters. The total integration within the cortex increased from the WR to the SD state, but not within all networks (*bold white italics depict significant changes, FDR corrected*). **(C)** The change in total integration at each level of the hierarchy mapped onto the cortical surface illustrates the increase in integration is most focused toward the centre of the lateral surface.



[NC1]

Fig 2. (A) There is a robust relationship between the change in total integration across the cortex and decrement in both performance accuracy and speed across three cognitive tasks from the WR to the SD state (top panel; performance on the x-axes is depicted as the first component from a principal component analysis on task outcomes). The paired change in integration and performance was also observed for recovery after the nap (bottom panel). **(B)** Total integration increased on average from RW to SD, but there was a drop during the recovery nap despite remaining high upon waking after the nap (lines represent significant within-subjects differences between sessions). **(C)** Conversely, the functional clustering ratio (FCR) also increased on average from RW to SD, however significantly increased in all subjects during the nap containing NREM sleep, indicating the role of FCR in conscious states (lines represent significant within-subjects differences between sessions).

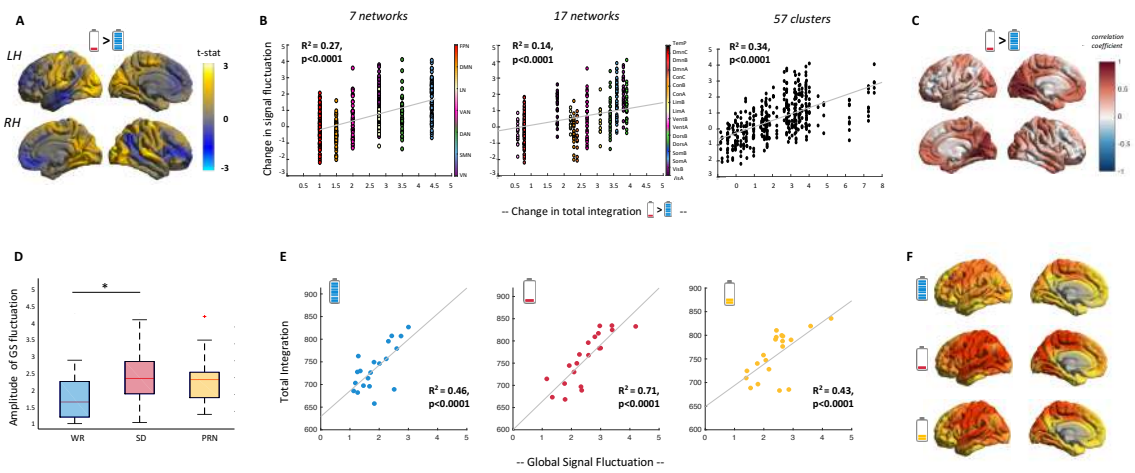


Fig 3. The relationship between functional integration and local and global signal fluctuations. **(A)** The group-average change in amplitude of the signal fluctuation (std deviation of signal) in each of 400 cortical parcels between SD and WR states. (**B)** Correspondence between the group-average change in amplitude of signal fluctuation with group-average total integration within 7 networks, 17 networks, and 57 clusters (significance corrected with 100 spin permutations). **(C)** The individual-level relationship between change in amplitude of the signal fluctuation and integration within 17 networks. **(D)** The group-average amplitude of the global signal fluctuation in the WR, SD and PRN states. **(E)** Relationships between total integration across the cortex and the amplitude of the global signal fluctuation in the WR ( ), SD ( ), and PRN ( ) states. **(F)** Correlation between each parcel's timeseries and the global signal in each state.

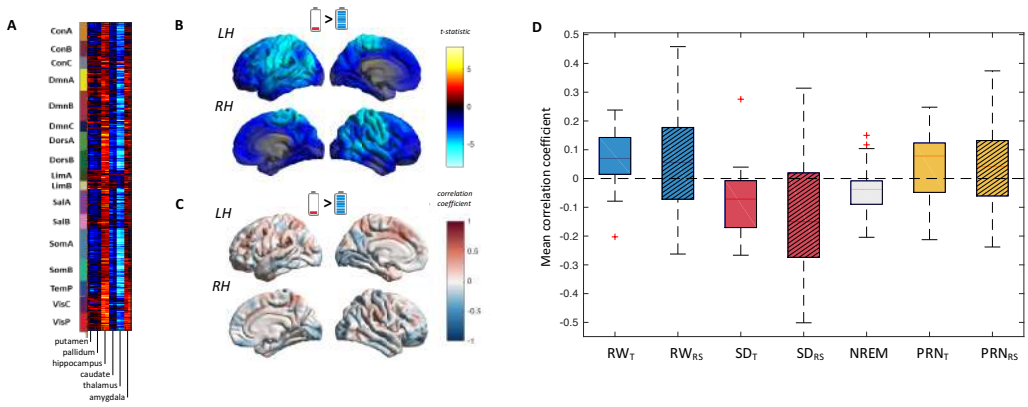


Figure 4. Changes in thalamocortical connectivity and the relationship to functional integration. **A** The group-average change in connectivity (correlation of signals) between all 400 cortical parcels and 6 subcortical regions from sleep deprivation (SD) and well rested (WR) states. **B** Spatial map of changes in thalamocortical connectivity between SD ( ) and WR ( ) states. **C** The individual level relationship between change in thalamocortical connectivity and integration within 17 networks. **D** The group-average strength of thalamocortical connectivity in the WR, SD and PRN states.