Effector-independent brain network for auditory-motor integration: fMRI evidence from singing and cello playing

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Highlights

- Expert cellists were asked to compensate for or ignore introduced pitch perturbations when singing/playing during fMRI scanning.

- Cellists were able to sing/play target tones, and compensate for and ignore introduced feedback perturbations equally well.

- Brain activity overlapped for singing and playing in IPS and SMG when compensating, and pSTG and dPMC when ignoring.

- Differences between singing/playing across were most prominent in M1, centered around the relevant motor effectors (hand, larynx)

- Findings support the hypothesis that pitch regulation during cello playing relies on structures within the singing network with differences arising primarily at the level of forward motor control

Abstract

Many everyday tasks share high-level sensory goals but differ in the movements used to accomplish them. One example of this is musical pitch regulation, where the same notes can be produced using the vocal system or a musical instrument controlled by the hands. Cello playing has previously been shown to rely on brain structures within the singing network for performance of single notes, except in areas related to primary motor control, suggesting that the brain networks for auditory feedback processing and sensorimotor integration may be shared (Segado et al. 2018). However, research has shown that singers and cellists alike can continue singing/playing in tune even in the absence of auditory feedback (Chen et al. 2013, Kleber et al.

2013), so different paradigms are required to test feedback monitoring and control mechanisms. In singing, auditory pitch feedback perturbation paradigms have been used to show that singers engage a network of brain regions including anterior cingulate cortex (ACC), anterior insula (aINS), and intraparietal sulcus (IPS) when compensating for incorrect pitch feedback, and posterior superior temporal gyrus (pSTG) and supramarginal gyrus (SMG) when ignoring it (Zarate et al. 2005, 2008). To determine whether the brain networks for cello playing and singing directly overlap in these sensory-motor integration areas, in the present study expert cellists were asked to compensate for or ignore introduced pitch perturbations when singing/playing during fMRI scanning. We found that cellists were able to sing/play target tones, and compensate for and ignore introduced feedback perturbations equally well. Brain activity overlapped for singing and playing in IPS and SMG when compensating, and pSTG and dPMC when ignoring; differences between singing/playing across all three conditions were most prominent in M1, centered on the relevant motor effectors (hand, larynx). These findings support the hypothesis that pitch regulation during cello playing relies on structures within the singing network and suggests that differences arise primarily at the level of forward motor control.

Keywords: auditory-motor integration, singing, cello playing, fMRI, auditory-vocal integration, motor control

1 Introduction

Maintaining a correct musical pitch when singing or playing an instrument is a complex sensory-motor skill whose success depends on feed-forward motor control, auditory feedback integration and error correction (Zatorre et al. 2007; Kleber and Zarate 2014). The brain networks underlying auditory-motor integration have been explored in speech and singing (Kleber and Zarate 2014; Rauscheker 2011; Hickok and Poeppel 2004; Tourville and Guenther 2011), but it is not yet known whether the same neural systems underlying vocal control are also engaged for skills like playing instruments, that have common high-level sensory goals to singing, but are phylogenetically newer and depend on very different movements and effectors.

Studies that have separately investigated the brain regions contributing to musical instrument playing and singing often report activation in similar functional networks (Zatorre, Chen, and Penhune 2007; R. M. Brown, Zatorre, and Penhune 2015, Kleber and Zarate 2014). More importantly, a recent fMRI study from our laboratory directly compared singing and cello

playing within the same individuals and found that the networks for simple feed-forward control

were almost entirely overlapping (Segado et al. 2018). This finding raised the possibility that

musical instrument playing may make use of the same auditory-motor networks as vocalization,

consistent with the concept of neuronal recycling (Dehaene 2005). However, our previous study

examined simple playing and singing, which only engages the feed-forward component of

auditory-motor control. A hallmark of auditory-motor integration in the vocal system is feedback

control, where auditory feedback is used to modulate the motor response to correct or maintain

the appropriate pitch (Burnett et al. 1998). Therefore, the current study again compares singing

and cello-playing but uses a pitch perturbation paradigm to test whether similar feedback control

and error correction mechanisms are engaged for the two instruments.

Behaviourally, it has been clearly demonstrated that monitoring of auditory feedback is

essential for both singing and playing in tune (J. Chen et al. 2008; Kleber and Zarate 2014).

Research on pitch stability in expert cellists during shifting movements has been shown to

require ongoing auditory feedback in order to continue producing sequences of notes in tune (J.

Chen et al. 2013). Similarly, research on singing has shown that pitch is less accurate and more

variable in the absence of auditory feedback (Kleber et al. 2017). However, with sufficient

expertise, people can sing and play musical instruments with a high degree of accuracy even

when auditory feedback is attenuated (Kleber et al. 2017; J. Chen et al. 2008; Zarate and Zatorre

2008, 2005), likely based on highly developed forward models (Kleber et al. 2013) combined

with somatosensory, kinesthetic, and vibrotactile cues (Askenfelt and Jansson 1992; Goebl and

Palmer 2008).

Auditory feedback perturbation paradigms, which isolate the effects of auditory feedback

on behaviour from those of feedback received through somatosensory modalities, have been used

extensively to characterize the role of auditory feedback in auditory-vocal integration. In speech

and non-speech vocalizations, it has been shown that participants will reflexively compensate for

a variety of auditory feedback perturbations including loudness (Lane and Tranel 1971) and pitch

(F0) (Tourville, Reilly, and Guenther 2008). Both of these reflexes are also seen during non-

speech vocalization in a variety of non-human animal models as well (J. Luo, Hage, and Moss

2018). A compensatory response to perturbed pitch feedback has also been observed during

singing, with research showing that participants compensate for introduced pitch perturbations

both when holding a constant pitch (Burnett et al. 1998) and when executing dynamic pitch

changes (Burnett and Larson 2002), and that a rapid compensatory response may be involuntary

(Zarate, Wood, and Zatorre 2010). Research asking participants to ignore auditory feedback

perturbations, thereby requiring them to rely primarily on a forward model, has been especially

useful in understanding the role of expertise, and has revealed that expert singers are better able

to ignore both incorrect pitch (Zarate and Zatorre 2005, 2008) and loudness (Tonkinson 1994)

auditory feedback than nonsingers.

Figure 1 Select components of Feedforward and Feedback networks | Feedforward regions encompass those related
to motor planning (SMA/pre-SMA, dPMC), motor execution (M1 Hands, M1 Larynx). Feedback regions encompass
those related to feedback monitoring (STG, including HG) and auditory-motor integration (IPS, SMG).

Accompanying the behavioural evidence that auditory feedback is used to guide

movements for vocal pitch regulation are models that describe the brain networks used for motor

planning and execution, auditory feedback processing, and auditory-motor integration (Figure 1).

The feedforward component includes primary motor, dorsal pre-motor, and supplementary motor

cortices (M1, dPMC, SMA) and parts of the cerebellum related to the orofacial articulators

(Zatorre 2007; Kleber and Zarate 2014; Rauscheker 2011; Hickok and Poeppel 2004; Tourville

and Guenther 2011). Specific regions within M1 vary based on the effector used to accomplish

the task with some areas controlling the orofacial articulators (S. Brown 2008) including the

larynx, and others controlling bilateral hand movements (Yousry et al. 1997; Lotze et al. 1999).

In the vocal system, the periaqueductal gray (PAG), a brainstem nucleus that directly innervates

the larynx, has also been found to regulate the initiation of voluntary vocalizations (Larson 1991;

Dujardin and Jurgens 2005; Jurgens and Ploog 1970). Auditory feedback processing has been

shown to involve primary and secondary auditory regions, including Heschl's gyrus (HG),

posterior superior temporal gyrus (pSTG) and superior temporal sulcus (STS). Auditory-motor

integration has been linked to pSTG, supramarginal gyrus (SMG), inferior parietal lobule and

intraparietal sulcus (IPL, IPS), as well as the anterior insula and anterior cingulate cortex (aINS,

ACC) (Zatorre 2007; Kleber and Zarate 2014; Rauscheker 2011; Hickok and Poeppel 2004;

Tourville and Guenther 2011). In particular, in a study examining auditory-motor integration

during singing, a network involving IPS, SMG, STG/STS, aINS, and ventral pre-motor cortex

(vPMC) was found to be engaged when successfully ignoring large pitch feedback perturbations

(Zarate and Zatorre 2008), while the ACC and pSTS were found to be engaged during

involuntary correction of small pitch shifts (Zarate, Wood, and Zatorre 2010).

The roles of feedforward and feedback brain networks have also been investigated during

musical instrument playing. A study on pitch and timing feedback manipulations during

keyboard playing found that participants recruited both feedforward (SMA, cerebellum) and

feedback (areaSpt, IPL, ACC) areas to a greater extent when pitch feedback was perturbed

compared to simply playing a simple melody (Pfordresher et al. 2014). While this study did not

allow for the online pitch corrections that occur during continuous pitch instrument performance,

this finding still demonstrates that these brain structures are linked to the sound-to-movement

transformations necessary for using incorrect pitch feedback to plan future movements. In

addition, several studies have found that when participants with no musical training learn to play

simple sequences on the keyboard, they quickly form a link between sounds and movements,

which is reflected in coordinated activation of motor and sensory brain regions even when only

sensory input is provided (J. L. Chen, Zatorre, and Penhune 2006; Stephan, Lega, and Penhune

2018; Lahav et al. 2005; Herholz et al. 2015).

While keyboard studies cannot directly address the role of these structures in pitch

regulation since the keyboard is a discrete-pitch instrument, the same finding has recently been

replicated on the cello, which like the voice has a continuous pitch distribution. When novices

learned to play a set of simple cello sequences they recruited the auditory to dorsal-cortical
pathway after only one week of cello learning compared to the pre-training (Wollman et al.
2018). Moreover, correlated activity between auditory cortex and SMA/pre-SMA after one week
of training was found to be predictive of better learning outcomes after 4 weeks of training. The
latter finding in particular speaks to the functional importance of sensory-motor links in the
production of accurate pitch sequences.

While much is known about the brain networks used for auditory-motor integration,
especially for vocalization, the functional role of some brain structures in pitch regulation has not
been fully characterized. One such structure is the pSTG. It has been shown that pSTG activity is
attenuated in anticipation of self-generated sounds (Bendixen, SanMiguel and Shroger 2012;
Mathias, Gehring, and Palmer 2019; Christoffels, Formisano, and Schiller 2007), however
studies have also shown that activity in auditory cortex is stronger when listening to sounds
produced on the instruments for which one has the greatest expertise (Gebel et al., 2013), and is
stronger for expert singers than for non-singers (Zarate and Zatorre, 2008), suggesting that
expertise may result in enhanced auditory processing in this area (Reznik et al 2014). Another
brain structure whose role is likely critical in sensory-motor mapping is the IPS, which is
recruited for high-level pitch transformations even in the absence of a motor performance task
(Foster 2010; Albouy et al 2017), but has also been shown to be mapped topographically
according to the movements necessary to accomplish tasks like reaching and grasping (Culham
and Valyear 2006, Grefkes and Fink 2005).

In the present study we directly investigate whether singing and cello playing use similar
or distinct networks of brain regions for pitch regulation. To do this, trained cellists performed a
pitch-feedback perturbation paradigm designed to test both the feedforward component of the
auditory-motor integration network (ignoring pitch perturbations), and the feedback component
(compensating for pitch perturbations). All participants performed both tasks to allow for direct
comparisons between cello playing and singing within the same individuals. For the cello
playing task, cellists played a fully MR compatible cello device (Hollinger and Wanderley 2013,
2015) used in our previous research (Wollman et al. 2018). This paradigm allows us to answer
specific questions about the role of key brain structures within the singing network. For the IPS,
if singing and cello playing overlap directly when compensating for pitch perturbations, then it
would support the hypothesis that at least one role of the IPS in pitch regulation is to accomplish

high-level pitch transformations, whereas if they are completely separate it would support the

hypothesis that its role is to carry out sensory-to-motor transformations specific to the effector

needed to accomplish the task. For the pSTG, contrasting the activity for these two instruments

will allow us to test the hypothesis that cello expertise results in enhanced processing for cello

playing relative to singing, or that activity is attenuated for both cello playing and singing due to

the anticipation of a self-generated sound. More generally, the present study will allow us to

extend existing theories about cortical representation of complex skills, including the theory of

neuronal recycling, by testing whether pitch regulation during instrument playing, a human-

specific cultural task, uses phylogenetically ancient brain networks that exist for vocal pitch

regulation.

2   Materials and methods

2.1   Subjects

A total of 15 expert cellists (10 female) were recruited from the Montreal community.

They reported normal hearing, no neurological disorders, and had no contraindications for the

MRI environment. Thirteen participants (9 female) were included in the final analysis (mean

years experience = 12.93 ± 4.46, mean starting age = 9, mean practice hours per week = 12.07);

two were excluded from the analysis due to technical problems. This study was approved by and

carried out in accordance with the recommendations of Montreal Neurological Institute Research

Ethics Board and the McConnell Brain Imaging Centre. All subjects gave written informed

consent in accordance with the Declaration of Helsinki.

2.2   Experimental Paradigm

2.2.1   Task Conditions

There were three main task conditions (Compensate, Ignore, and Simple) for each of two

instruments (Cello, Singing). In each of the three conditions, participants were presented with a 1

s auditory target tone that they were instructed to sing or play back for 2.5 s (Figure 2A).

Participants heard both the auditory targets and the auditory feedback of their own performance

binaurally through insert earphones. A pink-noise background was used to mask bone

conduction so that participants could only use the auditory information provided through the

earphones to the greatest extent possible. For Compensate and Ignore trials (40% of trials, 240

total), between 1 and 1.5 s after participants started singing/playing back the target, the pitch of

their auditory feedback was shifted up or down by 100 cents (one semitone) in an unpredictable

manner (jittered up to 500 ms). On Compensate trials, participants were instructed to make a

compensatory movement in order to go back to hearing themselves sing/play the correct (target)

tone (Figure 1B). On Ignore trials, participants were instructed to avoid making any

compensatory movements, and to continue singing/playing the target tone even though its pitch

would sound shifted in their earphones (Figure 2B). The Simple condition comprised the subset

of trials within the Compensate or Ignore conditions where no shift was introduced (20% of

trials, 120 total) and thus participants simply had to sing or play back the presented target tone

without perturbation.

Three additional control conditions were included in this experiment: Masked Feedback,

Listen, and Rest. In the Masked Feedback condition (20% of trials, 120 total), participants were

presented with the same target tones as in the Simple/Compensate/Ignore conditions and were

asked to sing/play them back but they received only pink masking noise through the earphones.

For Listen trials (13.33% of trials, 80 total) participants were visually cued to listen, and the

auditory target tone was followed by a 2s pre-recorded, non-pitch shifted playback of that target.

Participants were instructed to listen to the playback of the tone without making any movements

or sounds. For Rest trials (6.67% of trials, 40 total) participants were visually cued to rest, and

were instructed to not move or make any sounds.

2.2.2   Stimuli

Presented target tones corresponded to pitches from the Western music scale E3, F#3, for

cello, and E3, F#3, or E4, F#4 (one octave higher) for singing depending on the participant's

vocal range. Tones were recorded by either a female vocalist, male vocalist, or on a cello.

Female participants heard and imitated female voices, male participants heard and imitated male

voices. At the start of each session, sound levels were set to default values of 78.3db SPL for

pink masking noise and 15.6 dB above the noise floor for auditory targets. Volume settings were

adjusted on a per-subject basis such that masking noise and auditory targets were presented at a

comfortable volume and that masking noise attenuated non-pitch shifted feedback to the greatest

extent possible. To determine this volume level, a pitch shift of 100 cents was applied and

participants would sing/play a constant note while the experimenter adjusted the volume until

participants reported only hearing the pitch shifted note through their earphones. The position of
volume knobs was noted for the subsequent fMRI session.

2.3   Experimental Design

The experiment comprised 10 fMRI runs, each of which had 4 blocks of 15 trials. Each
block was made up of a single condition (Compensate, Ignore, Masked Feedback) divided into
sets of 6 trials on each instrument (cello, singing).   Each set of 6 trials was preceded by 1 Listen
trial, and a single Rest trial was included at the end of each block (Figure 2C). The order of
instructions and instruments was counterbalanced across runs, and the pitch perturbation (2 no-
shift, 2-shift up, 2-shift down) was pseudo-randomized within Compensate/Ignore blocks.

A sparse sampling paradigm was used for the fMRI session (Belin et al. 1999), where a
long delay in TR was used to allow tasks to be carried out in the silent period between functional
volume acquisitions, thus minimizing acoustical interference. Sparse sampling can also reduce
movement-related artifacts since the scanning takes place after the motor production for each
trial. The start time of individual trials was jittered up to 500ms to increase the likelihood of
catching the peak of the haemodynamic response.

Figure 2 Task and Conditions | A) Example of one experimental trial. Sparse sampling design used to avoid auditory
and motion artifacts. Auditory target presentation, instruction presentation, and singing and cello playing were done
during the silent period between scans B) Typical behavioural response to pitch feedback perturbation when

participants were instructed to Compensate (left) or to Ignore (right) for an introduced pitch perturbation of 100
cents (arrow indicates shift onset) C) Example of one 15-trial Compensate block. Instrument and Condition were
counterbalanced across runs, and note/pitch perturbations were pseudorandomized within each block. Simple
condition trials (perturbation magnitude 0 cents) were interspersed within Compensate/Ignore blocks.

2.3.1   Procedure

To allow participants to adjust to the fMRI-compatible cello and the constraints of

playing it in the scanner, each person underwent a 10 min familiarization session no more than 1

week prior to their session in the MR scanner. During the familiarization session each participant

was asked to lie inside a structure that simulated the space constraints of the MRI environment.

For both the familiarization session and the fMRI session, a microphone was suspended

approximately 5 cm from the mouth, the MRI compatible cello device was placed along the torso

using a specialized support, and bilateral sound delivery was provided via insert earphones

(Sensimetrics, Dayton Audio DTA-1 amplifier). The microphone and cello were connected to a

Zoom F8 portable field recorder, and to a midi controlled TCHelicon VoiceOne pitch shifter.

The shifter was used to shift the pitch feedback on some trials, or mask the feedback on other

trials (Figure 3). All participants were asked to play both target notes on the cello and to sing

both target notes, and to try warming up as they would on a regular instrument.

Within 1 week of the familiarization session, participants were tested in the Siemens Trio

3T magnetic resonance (MR) scanner at the Brain Imaging Center of the Montreal Neurological

Institute. Each participant was fitted with MR-compatible earphones. The MR-compatible

microphone was attached to the mirror support system and the MR-compatible cello was laid

across the torso using a special MR-compatible stand that prevented it from moving during task

performance.

2.3.2   MRI Acquisition

During the 10 functional runs, one whole-head frame of 28 contiguous T2*-weighted

images were acquired (Slice order = Interleaved, TE = 85ms, TR = 6.7s, Delay in TR = 4.4s, 64

$\times$ 64 matrix, voxel size = 4mm^3). All tasks were performed during the 4.4s silent period between

functional volume acquisitions. On each trial, the target tone was delivered for one second

together with the visual instruction; the rest of the trial was taken up by reproduction of the cello

277 or sung tone, or by no action on Rest trials (See Figure 2B). A high-resolution whole-brain T1-
278 weighted anatomical scan (voxel size = 1mm^3) was collected between runs 5 and 6.

2.3.3   Behavioral Analyses

Individual trials of singing and cello playing were analyzed using the pitch information
extracted from the recorded audio signals. Each trial's audio was first segmented from the
continuous 6-track audio using Audacity software. The trials were then processed using a custom
analysis pipeline implemented in Python, with a GUI for visualizing and optimizing analysis
parameters.

The ambient noise in the scanner room had a peak resonance of 160 Hz that interfered
with the extraction of fundamental target pitches, so harmonics 3–10 of the cello and singing
tones were used for pitch extraction. To reject room noise and to isolate the harmonics of
interest, the raw microphone signal was high-pass filtered with a cutoff at 367 Hz and low-pass
filtered with a cutoff at 4,216 Hz. Pitch estimation was then performed using the YinFFT
algorithm provided in the Python module Aubio (Brossier 2007), producing a time-series of pitch
estimations (detected harmonic, in Hz) and confidence ratings (between 0 and 1). Estimates were
adjusted to their representative fundamental pitches before selecting stable pitch regions for
further analysis. Stable pitch regions were defined as: segments of at least 150 ms in which the
rate of change of the pitch did not exceed 100 Hz/s (or approximately 0.07 Hz per 32-sample
pitch estimation window at the sampling rate of 44,100 Hz). Of these regions, only those that
maintained a confidence rating of at least 0.7 according to the algorithm were included. Trials
were rejected if no regions were found to meet the stability and confidence criteria, if
participants started playing after the pitch shift was introduced, or if they stopped playing before
the end of the trial. In total, 86.5% of trials were retained. Rejected trials were excluded from the
fMRI analysis.

Pitch extraction was performed for both the unshifted raw output track (produced) and for

the shifted headphone track (perceived) to allow for a direct comparison between the produced

and perceived audio. Our main outcome measure, deviation from the expected tone, was

calculated as the difference between the produced tone and the target tone (expressed in cents, or

100[ths] of a semitone) within three 150ms windows relative to shift onset (0 ms): Pre-Shift (- 150

ms to 0ms), Early Post-Shift (150 ms to 300ms), and Late Post-Shift (1000 ms to 1150 ms) for

each of the Simple, Compensate, and Ignore conditions (Equation 1). Because we had no specific

hypotheses related to the directionality of these perturbations, upwards and downwards

perturbations were treated as equivalent, and values from the downwards perturbation were

therefore multiplied by -1.

315
$$cents = 1200 * log_2\left(\frac{Freq_{produced}}{Freq_{target}}\right)$$

Equation 1 Conversion from absolute frequency difference to normalized cent difference

In addition to the trial-by-trial pitch traces, a global measure of accuracy for each

participant was calculated to examine the relationship between overall performance and brain

activity. This measure was determined by averaging the cent deviation from the target tone at

the Pre-Shift and Late Post-Shift timepoints, including the Simple condition when no pitch shift

was introduced so as to account for any natural drift in pitch throughout the trial. For the

Compensate condition, perfect performance was considered to be 100 cents in the direction

opposite to the introduced pitch perturbation, whereas for the Ignore condition perfect

performance was considered to be 0 cents deviation from the target tone. In order to examine

BOLD activity as a function of task performance, scores across trials for each condition were

averaged to give a global participant score, which was used in the regression analyses.

2.3.4 fMRI Analyses

fMRI data were analysed using the FSL6.0 FEAT toolbox (Jenkinson et al. 2012). Brain

extraction was carried out using BET2. Functional volumes were aligned to the high resolution

anatomical and then to MNI152 1mm standard space using FLIRT non linear registration with 12

degrees of freedom and a warp resolution of 10mm. To improve the registration quality, b0

unwarping was carried out using a percent signal loss threshold of 50%. Motion parameters were

estimated using MCFLIRT, and fMRI time course was temporally filtered to remove drifts

greater than 160 ms. To further decrease the number of motion-related active voxels outside the

brain, a brain mask based on the MNI152 1mm brain was applied prior to thresholding. To boost

the signal to noise ratio, images were spatially smoothed with an 8 mm FWHM kernel. FLAME-

1 mixed effects modeling was used to fit the GLM to the fMRI signal.

Statistical significance was determined using an FSL cluster probability threshold of $p <$

0.05 with a voxel-wise significance level of $z = 2.3$ ($p < 0.05$). The cluster probability threshold

serves as a correction for multiple comparisons. A total of 21 contrasts were carried out.

Contrasts were carried out for each of the instruction conditions (simple vs rest, compensate vs

simple, and ignore vs simple) within each of the instruments (singing, cello playing). Additional

contrasts were carried out to directly compare the two instruments within each of the instruction

conditions (e.g. singing compensate vs cello compensate), and between instruction conditions

([singing compensate vs ignore] vs [cello compensate vs ignore]). Additionally, task

performance (on a per-subject basis) was regressed against the BOLD signal for each of these

contrasts to determine whether or not activity in these areas is positively correlated with good

performance on the task, as would be expected if the region in question is specifically linked to

the cognitive/motor demands of the task of interest. Statistical conjunctions were carried out to

identify commonalities in singing vs cello playing, using the conjunction script created by the

Warwick University Department of Statistics, which also made use of the FSL tools (Nichols et

al. 2005). This script carries out a voxel-wise thresholding of $p < 0.05$ in both conditions of

interest, and then carries out a cluster correction of $p < 0.05$.

Functional Connectivity analyses were carried out using the FSL6.0 FEAT toolbox

(Jenkinson et al. 2012). A seed region in the region of primary auditory cortex [Heschl's Gyrus

(HG)] was identified by masking the conjunction of singing and cello playing from the

functional data with an anatomically defined mask (Harvard Structural Brain Atlas). The

activation time course in the HG seed was extracted and correlated with the whole-brain time

course for each task of interest, which was estimated using the GLM. Correlated voxels were

thresholded as described above. Regions that showed a correlated time course were then

correlated with task performance to determine whether those areas were contributing directly to

good performance on the task.

3   Results

3.1   Behavioural Findings

To determine how accurately participants were able to match the target tone, pitch was

averaged across all three timepoints within the simple condition and the cent deviation between

the average pitch and the target tone was computed (mean $= 0.86 \pm 0.27$ cents). A 3-way anova

(3 condition x 3 timepoints x 2 instrument) was carried out to determine the extent to which

participants could compensate for introduced pitch perturbations and also the extent to which

they could ignore them both when singing and playing the cello. There were significant main

effects of condition ($F_{(2,215)}=324.55$, $p<0.0001$) and timepoint ($F_{(2,215)}=332.73$, $p<0.0001$)

driven by a highly significant condition x timepoint interaction ($F_{(4,215)}=121.06$, $p<0.0001$).

While a main effect of instrument ($F_{(2,215)}=8.448$, $p=0.004$) was observed due to an overall

magnitude difference, this difference did not affect the pattern of results within the key

comparisons. There was no instrument x condition interaction ($F_{(2,17)}=324.55$, $p<0.0001$), no

instrument x timepoint interaction ($F_{(2,215)}=0.31$, $p>0.73$), and no instrument x condition x

timepoint interaction ($F_{(4,215)}=0.068$, $p>0.99$). To explore the condition x timepoint

interactions, a 2-way anova was carried out for each instrument (Figure 4).

Figure 4 Deviation from target tone during simple, compensate, and ignore conditions | Deviation from target tones
at three 150ms windows (Pre-shift, Post-early, Post-late) relative to pitch perturbation onset (0 ms) for singing (top)
and cello playing (bottom) as heard through the participant's headphones. In simple, cmp, and ign circles, black
trace represents what participants heard through headphones and grey trace represents what participants produced.
For the Simple condition where no shift was introduced the 'shift' was considered to be at the midpoint of the trial.
For Compensate and Ignore conditions, perturbation was 100 cents. Significance stars refer to cent change from the
previous time point.

3.1.1 Singing

The 2-way anova for singing (Figure 4 top subplot) showed a main effect of condition

$(F(2,107)=125.4, p<0.0001)$ and timepoint $(F(2,107)=138.2, p<0.0001)$ and a significant

condition x timepoint interaction $(F(4,107)=51.79, p<0.0001)$. Pairwise multiple comparisons

were carried out using Tukey's HSD to test the effect of timepoint across and within each

conditions. There were no significant differences across conditions at the pre-shift timepoint

[simple vs ignore $(F(2,107)=125.4, p=0.82)$, simple vs compensate $(F(2,107)=125.4, p>0.99)$, or

compensate vs ignore $(F(2,107)=125.4, p=0.83)$], demonstrating that participants were all able to

match the target tone before the manipulation was introduced $(mean_{pre}=0.86 \pm 18.09$ cents).

Across conditions for the early post-shift timepoint, we found a significant difference for simple

vs ignore $(F(2,107)=125.4, p<0.0001)$ and simple vs compensate $(F(2,107)=125.4, p<0.0001)$,

but no significant difference for compensate vs ignore $(F(2,107)=125.4, p=0.93)$. This indicates

that 150ms following the introduced pitch shift, participants were equally affected by the pitch

change in the compensate condition ($\text{mean}_{\text{post-early(cmp)}}$=-87.51 ± 14.86) as in the ignore condition

($\text{mean}_{\text{post-early(ign)}}$=-88.86 ± 12.99).

Within the simple condition, no significant differences were observed for the comparison

of pre-shift vs post-early ($F(2,107)$=138.2, p=0.99) or post-early vs post-late timepoints

($F(2,107)$=138.2, p=0.84) showing that participants were able to sing a stable pitch when no

feedback manipulation was introduced ($\text{mean}_{\text{simple}}$ = -1.09 ± 19.42 cents). For the compensate

condition participants showed a significant pitch deviation from pre-shift to the early post-shift

timepoint ($F(2,107)$=138.2, p<0.0001) and then a significant reduction in deviation from the

early to the late post-shift timpoint ($F(2,107)$=138.2, p<0.0001), indicating that they both

responded to and were able to compensate for the perturbation. For the ignore condition,

participants showed significant pitch deviations for the early post-shift timepoint

($F(2,107)$=138.2, p<0.0001) that did not change for late post-shift timepoint ($F(2,107)$=138.2,

p=0.52), indicating that they responded to the perturbation and were able to maintain a stable

pitch in the face of conflicting feedback.

3.1.2   Cello Playing

The same set of analyses carried out for singing were also performed for cello playing

(Figure 4 bottom subplot). The results paralleled those observed for singing. The 2-way anova

showed a main effect of condition ($F(2,108)$=208.3, p<0.0001) and timepoint ($F(2,108)$=217.5,

p<0.0001) and a significant condition x timepoint interaction ($F(4,108)$=73.48, p<0.0001).

Pairwise multiple comparisons were carried out using Tukey's HSD to test the effect of

timepoint across and within conditions. There were no significant differences across conditions

at the pre-shift timepoint [simple vs ignore ($F(2,108)$=208.3, p=0.98), simple vs compensate

($F(2,108)$=208.3, p=0.95), or compensate vs ignore ($F(2,108)$=208.3, p=0.99)], demonstrating

that participants were all able to match the target tone before the manipulation was introduced

(mean_{pre}=-3.53±23.52 cents). Across conditions for the early post-shift timepoint, we found a

significant difference for simple vs ignore ($F(2,108)$=208.3, p<0.0001) and simple vs

compensate ($F(2,108)$=208.3, p=0.0001), but no significant difference for compensate vs ignore

($F(2,108)$=208.3, p=0.9579). This indicates that 150ms following the introduced pitch shift,

participants were equally affected by the pitch change in the compensate condition ($\text{mean}_{\text{post-}}$

$_{\text{early(cmp)}}$=-88.19 ± 14.92) as in the ignore condition ($\text{mean}_{\text{post-early(ign)}}$=-87.34 ± 15.76).

Within the simple condition, pitch was stable across all three timepoints with no

significant differences observed for the comparison of pre-shift vs post-early ($F(2,108)=217.5$,

$p>0.99$) or post-early vs post-late timepoints ($F(2,108)=217.5$, $p=0.86$) ($mean_{simple} = -1.83 \pm$

21.58 cents). Within the compensate condition, significant differences were observed in the

compensate condition for pre-shift vs post-early ($F(2,108)=217.5$, $p<0.0001$) and post-early vs

post-late timepoints ($F(2,108)=217.5$, $p<0.0001$). As when singing, participants compensated for

the feedback manipulation ($mean_{cmp} = -59.92 \pm 19.28$ cents) in the compensate condition, but

not in the ignore condition ($mean_{ign} = -3.77 \pm 16.84$ cents). There was a significant difference

between pre vs post-early timepoints ($F(2,108)=217.5$, $p<0.0001$) for the ignore condition, but

not for post-early vs post-late timepoints ($F(2,108)=217.5$, $p=0.70$). The compensate vs ignore

comparison was highly significant ($F(2,108)=208.3$, $p<0.0001$) in the post-late timepoint,

demonstrating that the introduced pitch perturbation directly influenced behaviour.

3.2   fMRI Findings

3.2.1   Simple tone reproduction

Consistent with previous findings (Segado et. al 2018), a statistical conjunction of cello

playing and singing compared to rest showed that both tasks recruited a bilateral network

including M1 and dPMC, as well as SMA and STG (Figure 5). Additionally, singing specifically

activated larynx area of M1, whereas Cello Playing recruited a region of M1 related to hand and

arm movements. Activity in larynx area of M1 was identified based on bilateral 10 voxel spheres

centered on the larynx area defined in Brown et al. 2006. Hand area was identified based on

bilateral 10 voxel spheres centered on hand knobs (Yousry et. al 1997).

Figure 5 Simple performance condition | A) Simple cello playing (orange), singing (blue) and conjunction (green).
B) Conjunction (green) and areas that were positively correlated with good task performance (pink). Singing and
cello playing were found to have overlapping activity in pre- post-central gyrus, STG and SMA. This activity was
found to be positively correlated with good performance on the task.

3.2.2   Compensation

Only trials where participants successfully compensated for the perturbation were

included in this analysis. When comparing the Shift to the Simple no shift condition both

singing and playing the recruited a bilateral network of regions in the dorsal-stream: dPMC, pre-

central gyrus, IPS, SMG extending to pSTG, and SMA extending to pre-SMA. These regions all

correspond to those of the auditory-vocal integration network reported previously for the

equivalent manipulation carried out in trained singers (Zarate et. al 2008). A statistical

conjunction of Sing and Play for the Compensate condition showed that similar regions of

SMA/Pre-SMA, dPMC, IPS, SMG were significantly active for both instruments (Figure 6A).

Regression analysis examining the relationship between compensation accuracy and BOLD

signal from the Compensate vs. Simple contrast in the regions of overlap showed that greater

activation in all of these regions was positively correlated with pitch accuracy (Figure 6B).

Figure 6 Compensating for pitch perturbations | A) Cello playing (orange), singing (blue), and Conjunction (green) of Compensate vs Simple contrast B) Areas within this conjunction (green) where activity is positively correlated with good task performance (pink) C) Cello playing > singing and D) singing > cello playing. Conjunction and regression show that SMA/pre-SMA, DPMC, SMG, and IPS are all contributing to good task performance in singing and in cello playing. Cello playing recruits more activity throughout the auditory motor integration network including in the BG and aINS. Singing shows more activity in vocal areas of motor cortex and cerebellum.

There were also significant differences observed between singing and cello playing in the
Compensate vs Simple contrast. Cello playing showed more, and more extensive activation in
bilateral dorsal motor and pre-motor regions extending posteriorly into the superior parietal
lobule as well as in the SMA, parietal operculum, the pre-cuneus and bilateral cerebellar Crus V
(Figure 6C). Singing preferentially recruited larynx area of M1, as well as cerebellar Crus I and
Crus II (Figure 6D).

3.2.3   Ignoring: similarities and differences

In the Ignore condition, singing and cello playing both recruited dPMC and STG when
contrasted with Rest (Figure 7A). The statistical conjunction of Sing and Play for the Ignore vs
Rest contrast showed overlapping activation in pSTG and dPMC. Regression analysis examining
the relationship between accuracy and BOLD signal from the Ignore vs. Simple contrast in the
regions of overlap showed that greater activation in pSTG was positively correlated with
performance score (Figure 7B).

As in the Compensate condition, cello playing elicited greater and more widespread
activation relative to singing throughout bilateral dPMC extending posteriorly to the superior
parietal lobule, in the SMA, the parietal operculum, and the pre-cuneus as well as in bilateral
Crus V, VIIIa and VIIIb of the cerebellum (Figure 7C). Singing showed greater activation in
larynx area and in Crus I/II of the cerebellum. In addition, singing showed greater activation in
bilateral hippocampus (Figure 7D).

Figure 7 Ignoring incorrect pitch feedback | A) Cello playing (orange), singing (blue), and Conjunction (green) of Ignore vs Simple contrast B) Areas within this conjunction (green) where activity is positively correlated with good task performance (pink) C) Cello playing > singing and D) singing > cello playing. Conjunction and regression show that only posterior STG is contributing to good task performance in both singing and in cello playing. Cello playing recruits more activity throughout the auditory motor integration network including in the BG and aINS, MFG, and IFG. Singing shows more activity in vocal areas of motor cortex and cerebellum, and in the hippocampus.

3.2.4   Functional Connectivity

Functional connectivity analyses were carried out for all three conditions to determine if brain activity in the region of primary auditory cortex [Heschl's gyrus (HG)] was correlated with activity in motor regions (or elsewhere) and, in doing so, determine whether multiple brain regions are working together in order to accomplish the experimental task (Figure 8). For both Sing and Play in all three conditions (Simple, Compensate, Ignore), activity in the HG seed was correlated with activity in bilateral STG within and around the HG seed, as well as with activity

in the SMA, and the dorsal part of M1. For singing, HG activity was correlated with activity in

regions of M1 corresponding to vocal articulators. For cello playing, HG activity was correlated

with activity in regions of M1 corresponding to hand knob (bilateral).

Figure 8 Functional connectivity from HG seed for cello playing (orange), singing (blue), and Conjunction (green) |
A) Simple condition B) Ignore condition and C) Compensate condition. In all three conditions, activity in auditory
cortex was correlated with activity in and around the HG seed as well as with activity in SMA and motor cortex.
Activity in motor cortex was effector-specific with singing recruiting larynx area and cello playing recruiting hand
area (both bilateral). In the compensate condition, only cello playing showed functional connectivity from HG to
cerebellum.

4   Discussion

The findings of this study support our main hypothesis that similar brain networks

underlie auditory-motor integration for singing and cello playing. First, the participants, who

were expert cellists but not expert singers, were all able to accurately match target tones in the

simple play or sing conditions and to accurately compensate or ignore auditory feedback

perturbations for both instruments. Second, the network of brain regions recruited for simple

singing and cello playing directly overlapped, except in primary motor cortex where activity was

observed in the larynx area for singing and the hand area for cello playing. Within the regions of

overlap, BOLD signal change in auditory cortex and functional connectivity from an HG seed to

a subset of these regions (STG, SMA, M1) were both positively correlated with pitch accuracy,

indicating that the synchronous activity of this network of brain regions positively contributed to

performance. Third, compensating for pitch perturbations when either singing or playing

recruited a bilateral dorsal network (dPMC, IPS, SMG, pSTG, SMA/pre-SMA). BOLD signal

change within all of these dorsal-stream regions was positively correlated with pitch

compensation performance. Further, activity in HG was temporally correlated with activity in a

subset of these regions (SMA, M1, STG) and bilateral Lobule VI of the cerebellum. Finally,

when ignoring pitch perturbations for both singing and cello playing participants recruited

overlapping regions in dPMC and pSTG. BOLD signal change and functional connectivity from

an HG seed to pSTG was positively correlated with pitch accuracy score. Taken together these

results indicate that there is a common network underlying auditory-motor integration that spans

vocal-motor and hand motor control. This conclusion is consistent with the neuronal recycling

hypothesis which posits that phylogenetically newer abilities dependent on human culture are

scaffolded on phylogenetically older capacities (Dehaene 2005).

4.1   Overlapping brain networks for singing and playing

Our first finding, that performance was highly accurate for singing and cello playing

across all three conditions (simple, compensate, ignore), is the first direct evidence showing that

the magnitude of the behavioural response to pitch feedback perturbations in continuous pitch

instruments is directly comparable to the response observed in singing. This finding is critical for

interpreting our neuroimaging findings, as it allows us to more confidently attribute the observed

similarities/differences in brain activity for these two tasks to specific brain networks, and not to

underlying behavioural differences.

In the simple play/sing condition, the contrasts of singing and cello playing compared to

rest, together with the conjunction analysis showed overlapping recruitment of brain areas

throughout dorsal motor regions and the STG, with overall greater activation for playing than

singing. We also observed expected differences in the location of motor activity, with singing

activating the larynx area to a greater extent than playing, and playing activating hand-motor

areas to a greater extent than singing. This is consistent with our previously published

neuroimaging finding showing substantial overlap in the auditory-motor network for single tone

reproduction when singing and playing (Segado et al. 2018).

The compensate and ignore conditions give complementary information related to the

feedforward and feedback components of the auditory-motor integration network, with the

compensate condition weighted towards regions that are involved in feedback integration. The

finding that cellists compensate as accurately when singing as they do on the cello is in line with

research showing that non-singers compensate as accurately for large pitch shifts as do expert

singers (Zarate 2008), and demonstrates that auditory feedback is sufficient for pitch regulation

in both tasks even when other sensory modalities (kinesthetic, vibrotactile) provide conflicting

information. For the compensate condition we found directly overlapping brain activation in the

IPS and SMG (part of the IPL) during singing and playing. The IPS and the IPL (including

SMG) are regions within the singing network whose role has not been fully characterized, as

they have been shown to be involved in both high level pitch transformations and also in

sensory-motor integration for vocal and non-vocal pitch regulation. Zarate et al. (2008) showed

that in singing the IPS and IPL (SMG) were recruited both when ignoring and compensating for

introduced pitch perturbations of 200 cents. A similar effect has also been shown in non-singing

vocalizations. Toyomura at al. (2007) showed recruitment of IPS and SMG when pitch feedback

was shifted while participants vocalized a steady vowel (/a/). The IPL has also been shown to be

recruited during a broad range of keyboard/piano playing tasks which require pitch feedback

monitoring. Perturbing pitch feedback during keyboard performance specifically elicited activity

in IPL (Pfordresher 2014), and activity in this region was found to be sensitive to the pitch

component of melody learning (Brown 2012). A more global role for the IPS in pitch-related

transformations is demonstrated by studies showing that it is engaged during performance of a

transposed melody discrimination task, and that the active region overlaps with that involved in

temporal re-ordering of pitches (Foster 2010, Foster 2013). It is therefore reasonable to speculate

that for tasks requiring very similar computations, in this case the transformation of pitch

feedback into a feed-forward motor command, similar infrastructure within the IPS would be
used.

In the present study we show that, within the IPS and IPL, cello playing and singing
recruit directly overlapping regions for the compensate condition. Within the IPS, overlap was
seen primarily in anterior portions of the IPS, which have been found to relate to sensorimotor
transformations and motor execution (Culham and Valyear 2006). This overlapping activity
extended ventrally to the IPL which, as mentioned above is consistently found to be active in the
musical instrument literature (Bangert 2006) at least in part due to its role in skilled object-
related actions like tool use (Binkofski, Klann, and Caspers 2016; Culham and Valyear 2006).
The mid to anterior localization of activity within the IPL is consistent with work showing that
these regions are most related to motor planning and execution, simple motor behaviours, tactile
reception, and a number of speech tasks like phonological short term memory (Tremblay, Shiller,
and Ostry 2003). Given this, it is reasonable to interpret our finding as evidence that vocal and
non-vocal tasks requiring pitch transformations for the purpose of movement planning, perhaps,
have similar underlying computations and are therefore carried out within the same region
largely independently of the source of auditory feedback and target motor effector. It is
nonetheless possible that the current paradigm and resolution of the scanning protocol was not
adequate to detect subtle differences in spatial locations of active regions, and that brain regions
are tightly adjacent as opposed to directly overlapping. However, that would still suggest an
organization within the IPS based on higher-level sensory transformations as opposed to motor
effector. This question could be addressed directly in the future using a multivariate analysis
technique like multivoxel pattern analysis that is more sensitive to differences between tasks
within a region of interest.

The findings from the ignore condition allow us to further determine the extent to which
singing and playing engage similar brain regions when auditory feedback is incorrect and
performance is, as a result, based on a forward model. We found that participants performed the
ignore task with as high a degree of accuracy when singing (for which they had no specific
expertise) as they did when playing (for which they had a very high level of expertise). This
finding suggests that the ability to successfully rely on a forward model is at least partly
independent of the effector used to accomplish a sensory goal, and may be more related to

feedback monitoring strategies than forward motor planning. We found that activity associated

with ignoring in the two instruments overlapped in dPMC and in pSTG, although there were also

separable activations in the motor hand area and the larynx area for playing and singing

respectively. Both dPMC and pSTG are consistently active in error monitoring and pitch control

tasks (Baumann 2005, S. Brown 2004), with dPMC being specifically relevant for associating

sounds with movements (Brown 2006) and pSTG being involved in error correction (Pfordresher

and Mantell 2014, Tourville and Guenther 2011). We found that activity in pSTG was positively

correlated with good performance, but activity in dPMC was not. Our interpretation of this

correlation is that the increased activity in auditory cortex resulted from the absence of the

typical inhibition of STG typically seen for monitoring of self-generated sounds (Bendixen,

SanMiguel, and Schröger 2012; Sanmiguel, Todd, and Schröger 2013; Mathias, Gehring, and

Palmer 2019; Christoffels, Formisano, and Schiller 2007). If participants were no longer linking

the perceived sounds to their produced output, and were instead increasing their reliance on a

forward model and on non-auditory sensory feedback, then it would follow that inhibition of

auditory cortex would be weaker and activity in pSTG would be stronger as a result. We would

therefore propose that the mechanisms involved in representing the target pitch stably in the face

of competing inputs, and perhaps inhibiting corrective responses, are shared for both singing and

cello, just as the mechanisms for compensation also appear to be shared.

4.2 Significance for feedforward and feedback control models

The extensive overlap observed for singing and cello playing across experimental

conditions suggests shared mechanisms that can be used flexibly for pitch regulation. One

interpretation is that, consistent with the theory of neuronal recycling, these mechanisms

originally developed for vocal control and are now being used for the purpose of pitch regulation

during instrument playing. The vocal pitch regulatory system, including several auditory-vocal

reflexes, are present in phylogenetically older species like non-human primates (Eliades and

Wang 2012), bats and frogs (J. Luo, Hage, and Moss 2018). Given that none of these species

play musical instruments (yet), they would have few if any uses for pitch regulation outside the

context of vocalization and it therefore seems reasonable to speculate that the brain mechanisms

governing vocal pitch regulation developed primarily for that purpose. However, a

complementary interpretation is that both vocal control and instrument playing make use of more

general-purpose feedforward and feedback mechanisms that are important for the control and

regulation of movement. Research done on visuomotor control has shown that error correction
may be best modelled as a Bayesian process (Kording and Wolpert 2004) with the strength of the
sensory prior, along with incoming sensory information, determining whether or not a corrective
action takes place. Such a framework has been shown to account the observation that expert
singers are better able to ignore incorrect pitch feedback while still showing a reflexive
compensatory response to small pitch shifts (Zarate 2010; Hahnloser and Narula 2017).

5   Conclusion

We found that cellists can perform pitch perturbation tasks as accurately when playing
the cello as when singing, and that playing/singing make use of directly overlapping brain areas
both when compensating for and ignoring introduced pitch perturbations. The functionally
connected network of overlapping brain regions includes those used for auditory feedback
processing and auditory-motor integration, but differs at the level of forward motor control. This
finding suggests that regions responsible for auditory-motor integration, like the IPS and SMG,
are performing high level sensory transformations as opposed to coding for specific motor
actions. Moreover, we found that the network of overlapping brain regions is consistent with the
singing network described in the literature, and with work done in auditory-motor integration
during musical instrument performance, further suggesting that brain networks for the two tasks
may be shared. We propose that this is due to a co-opting of brain mechanisms that developed
primarily for the purpose of vocalization, which is consistent with the neuronal recycling
hypothesis.

Author Contributions

666   The authors all contributed to the conception and design of the study. Melanie Segado
667 collected and analysed both the fMRI and behavioral data, including statistical analyses, and
668 wrote the first draft of the manuscript. All authors contributed to manuscript revision, read and
669 approved the submitted version.

Conflict of Interest Statement

671   The authors declare that the research was conducted in the absence of any commercial or
672 financial relationships that could be construed as a potential conflict of interest.

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