

Sterile Inflammation Alters Neutrophil Kinetics in Mice

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ABSTRACT – Neutrophils play a crucial role in establishing inflammation in response to an infection or injury, but their production rates, as well as blood and tissue residence times, remain poorly characterized under these conditions. Herein, using a biomaterial implant model to establish inflammation followed by *in vivo* tracking of newly formed neutrophils, we determine neutrophil kinetics under inflammatory conditions. To obtain quantifiable information from our experimental observations, we develop an ordinary differential equation-based mathematical model to extract kinetic parameters. Our data show that in the presence of inflammation resulting in emergency granulopoiesis-like conditions, neutrophil maturation time in the bone marrow and half-life in the blood reduces by about 40%, compared to non-inflammatory conditions. Additionally, neutrophil residence time at the inflammatory site increases by two-fold. Together, these data improve our understanding of neutrophil kinetics under inflammatory conditions, which could pave the way for therapies that focus on modulating *in vivo* neutrophil dynamics.

Conflict of Interest: The authors declare that they have no conflict of interest

1 INTRODUCTION

2 Neutrophils are short-lived cells of the immune system that play an essential role in pathogen
3 clearance and foreign body responses(1). They are continually produced in the bone marrow
4 through granulopoiesis, a process where hematopoietic stem cells (HSCs) differentiate to mature
5 neutrophils in sequential steps involving numerous intermediate progenitor populations(2, 3).
6 Mature neutrophils are recruited into circulation where their numbers remain relatively stable
7 throughout an individual's lifetime(3, 4). A delicate balance between progenitor proliferation,
8 maturation time in the bone marrow, half-life in the blood, and clearance at various tissue sites,
9 ensure that the numbers of neutrophils in circulation remain stable(5, 6).

10

11 The kinetics of neutrophil production, maturation, circulation, and death have been extensively
12 studied in humans and mice. In humans, over 10^{11} neutrophils are produced every day, and the
13 maturation time in the bone marrow and half-life in circulation has been measured to be about 6
14 days and 11-19 hours, respectively(7–9). In mice, the number of neutrophils produced is about 10^7
15 per day, their maturation time in the bone marrow is 2-3 days, half-life in circulation is 10-13
16 hours, and half-life at tissue sites range from 8-18 hours(6, 9–12). These measurements have been
17 made under steady-state, non-inflammatory conditions. Under inflammatory conditions, such as
18 during an infection, chronic disease, injury, or biomaterial implantation, neutrophil lifespans
19 remain unknown(13).

20

21 Herein, we use a mouse model of biomaterial implantation to determine the time for maturation of
22 neutrophils in the bone marrow, and blood and tissue residence time under sterile inflammatory
23 conditions. We track neutrophils spatially and temporally *in vivo* and mathematically model the
24 process to find that, in the presence of an inflammatory stimulus that results in a state resembling
25 emergency granulopoiesis, many parameters associated with neutrophil kinetics are altered.

26

27 **MATERIALS AND METHODS**

28 **Animal Studies**

29 All animal studies were conducted under the Control and Supervision Rules, 1998, of the Ministry
30 of Environment and Forest Act (Government of India), and the Institutional Animal Ethics
31 Committee, IISc. Experiments were approved by the Committee for Purpose and Control and
32 Supervision of Experiments on Animals (permit numbers CAF/ethics/546/2017 and
33 CAF/ethics/718/2019). Animals were procured from the Central Animal Facility, IISc or Hylasco
34 Biotechnology (India) Pvt. Ltd, Hyderabad, India (a Charles River Laboratory licensed supplier).
35 All experiments were performed on 8-14-week-old (weighing 20 – 30 grams) C57BL6 mice (both
36 female and male).

37

38 **Alginate and Chitosan microspheres**

39 Alginate and chitosan microspheres were prepared using a Spraybase® Electro spray system in a
40 sterile enclosure. Alginate microspheres - SLG20 alginate (Nova Matrix, FMC BioPolymer,
41 Drammen, Norway) was dissolved in 0.86% NaCl (saline) to a concentration of 1.4 % (w/v). This
42 solution was then passed through a 26G blunt needle, at the pressure of 0.5 bar and a voltage of 5
43 kV, into a 50 mM BaCl₂ cross-linking solution. The collector distance from the tip of the needle
44 was 5 cm. Chitosan microspheres - medium molecular weight chitosan (448877, Sigma-Aldrich,
45 USA) was dissolved in 1 % (v/v) acetic acid solution at a concentration of 1% (w/v) and stirred
46 overnight at room temperature (RT). The chitosan solution was then passed through a 26G blunt
47 needle at 0.8 bar pressure and a voltage of 6 kV, into 0.9 % (w/v) sodium tripolyphosphate cross-
48 linking solution (pH 5.0). The collector distance from the tip of the needle was 7 cm. All the
49 microspheres were collected and washed six times with sterile saline. The microspheres were then
50 incubated in 1% NaOH at RT, for two hours with a replacement of NaOH solution at one hour,
51 followed by incubation in a 1.6% (v/v) paraformaldehyde solution in phosphate-buffered saline at
52 RT for 1 hour. All microspheres were then washed with excess saline and distributed in 1.5 ml
53 sterile microcentrifuge tubes and sealed for use in implantation procedures.

54

55 **Surgical implantation of microspheres**

56 Microspheres were surgically implanted into the PC of mice as described(14). In brief,
57 microspheres (450 μ l) were suspended in 450 μ l sterile saline for implantation. The entire volume
58 (900 μ l) was then implanted into the PC following a laparotomy procedure. In controls (also called
59 mock controls), the animals went through the surgical procedure and were injected with 900 μ l
60 sterile saline.

61

62 ***In vivo* labelling of cells**

63 EdU was purchased from Carbosynth (UK). EdU was dissolved in sterile saline at a concentration
64 of 0.625 % (w/v), and each mouse received a concentration of 25 mg/Kg body weight(15) through
65 intraperitoneal injection using a 26G needle. Surgical procedures are also an inflammatory
66 stimulus. To exclude the inflammatory effects of surgery, we waited five days post-surgery to
67 inject EdU. At day 5, to label proliferating cells, 5-ethynyl-2-deoxyuridine (EdU) was injected
68 intraperitoneally (**Fig. S1**). Following EdU administration, mice were euthanized at 24-hour
69 intervals, and labeled neutrophils were quantified using flow cytometry.

70

71 **Retrieval of cells and microspheres**

72 Mice were anesthetized using ketamine solution to retrieve cells and microspheres. After
73 anaesthesia, about 500-1000 μ l blood was collected through the retro-orbital vein and cardiac
74 puncture. Next, mice were euthanized by cervical dislocation. Immediately following euthanasia,
75 5 ml of cold phosphate-buffered saline (PBS) with 4mM EDTA (PBS-EDTA) was injected into
76 the PC using a 26G needle. Through a small incision in the peritoneal wall, the fluid containing
77 cells was retrieved, passed through a 100 μ m filter (to filter out implants) and stored on ice before
78 analysis. Microcapsules were collected on the 100 μ m filter by rinsing the PC with PBS and stored
79 in 1.6% paraformaldehyde for analysis. Subsequently, the spleen and a tibia and femur (to get bone
80 marrow) were collected. A cell suspension was prepared by mincing the tissue using forceps and
81 passing the cell solution through a 100 μ m filter. Cells isolated from all sites (peritoneal fluid,
82 blood, bone marrow, and spleen) were subjected to RBC lysis and then counted manually using a
83 Bright-Line™ hemocytometer (0.1 mm).

84

85 **Flow cytometry**

86 For the quantification of labeled (EdU positive) neutrophils, after counting cells from each site,
87 0.5×10^6 cells were used for antibody staining and flow cytometry. First, cells were stained with
88 BD Horizon™ Fixable Viability Stain 510 for 20 mins at RT. Cells were then fixed using 1.6 %
89 paraformaldehyde for 30 mins at RT. Following one wash with excess PBS, cells were stained to
90 estimate EdU positive cells using Sulfo-Cyanine5 azide (Lumiprobe, USA) as per the
91 manufacturer's instructions. Following two additional washes with PBS, cells were stained with –
92 the monoclonal antibody against Ly6G (clone 1A8, BD Biosciences, USA) for 30 mins at 4°C, in
93 PBS containing 1 % BSA and 4 mM EDTA (staining buffer). Finally, cells were re-suspended in
94 staining buffer.

95

96 To monitor neutrophil activation markers in untreated mice, 0.5×10^6 cells from each site were
97 stained immediately with a combination of the following antibodies for 30 mins at 4°C: CD11b
98 (M1/70), Ly6G (1A8), CD45 (30-F11) CD54 (3E2), CD62L (MEL-14), CD182 (V48-2310) all
99 purchased from BD Biosciences (USA). For *ex vivo* activation –, 0.5×10^6 cells from each site
100 were first activated using 5 µg/ml Cytochalasin B (C6762, Sigma-Aldrich, USA) for 5 mins and
101 5 µM fMLP (F3506, Sigma-Aldrich, USA) for 30 mins at 37°C and then stained with antibodies
102 as mentioned above. Cells were stained with propidium iodide (2 µg/ml), and PI-positive cells
103 were excluded to identify live cells.

104

105 To identify neutrophil progenitors, RBC were lysed and 2×10^6 cells from bone marrow and spleen
106 were stained with lineage cocktail antibodies: I-A/I-E (M5/114.15.2), CD49b (HMα2), NK-1.1
107 (PK136), CD11c (N418), Ly6C (HK1.4), Ly6G (1A8), CD3(17A2), CD127 (A7R34),
108 CD19(6D5), CD45R/B220 (RA3-6B2) and stem/progenitor cell markers, c-Kit (2B8), Sca-1(D7),
109 CD34(SA376A4) and CD16/32(93). Cells were stained with propidium iodide (2 µg/ml), and PI-
110 positive cells were excluded to identify live cells.

111

112 For all protocols, appropriate single color (using compensation beads, BD Biosciences) and
113 fluorescence-minus-one (FMO) controls (using cells) were used to compensate the data and gate

114 positive populations, respectively. Flow cytometry data were collected using a BD FACSCelesta
115 (Becton Dickinson, USA) and analyzed using FlowJo (Tree Star, Ashland, OR, USA)

116

117 **Myeloperoxidase (MPO) and elastase activity assays**

118 The following numbers of cells were used for these assays: bone marrow – 2×10^6 , blood - $0.2 \times$
119 10^6 , peritoneal fluid - 0.2×10^6 . These cells were seeded in a 96-well clear flat bottom plates. PBS
120 was then added to make up the volume of each well to 135 μ l. CTAB was dissolved in PBS at a
121 concentration of 0.5 % (w/v), and 15 μ l was added to each well to lyse the cells. The cells were
122 then incubated at 37°C for 30 mins. After the incubation period, the plate was centrifuged at 1000
123 RCF at 4°C for 10 min. to pellet down all the cell debris. Supernatant aliquots (100 μ l) were placed
124 in 0.5 ml protein low bind tubes and stored at -80°C.

125

126 MPO activity: Supernatants were used at different dilutions for measuring MPO activity. Diluted
127 supernatant (75 μ l total volume) from each sample was added to a 96-well transparent flat bottom
128 plate. 75 μ l of 3,3',5,5'-tetramethylbenzidine (TMB, T4444, Sigma-Aldrich, USA) was then added
129 to each well for 90 seconds, followed by the addition of 150 μ l of 1 M H₂SO₄ to stop the reaction.
130 The samples were then read on a 96 well plate reader at 450 nm. Standard samples with different
131 myeloperoxidase concentrations (from human polymorphonuclear leucocytes, 475591, Sigma-
132 Aldrich, USA) were prepared to obtain a standard curve in the range of 26-1333 mU/ml. MPO
133 activity in the samples was estimated by interpolation from the standard curve.

134

135 Elastase activity: Elastase activity was determined by the chromogenic substrate N-
136 Methoxysuccinyl-Ala-Ala-Pro-Val p-nitroanilide (M4765, Sigma-Aldrich, USA). Supernatants
137 were used for measuring elastase activity. Briefly, 20 μ l of supernatant was added to 80 μ l of 1
138 mM substrate in a 96-well transparent, flat bottom plate, and absorbance was measured at 405 nm
139 for 60 minutes. Standard samples with different elastase concentrations (from human leukocytes,
140 E8140, Sigma-Aldrich, USA) were prepared to obtain a standard curve in the range of 16-166
141 mU/ml. Elastase activity in the samples was estimated by interpolation from the standard curve.

142

143 Assuming that only neutrophils produce myeloperoxidase and elastase enzymes, the enzyme
144 content per neutrophils was calculated using the following formula:

145 96 well reaction volume = $V = 150 \mu\text{l}$, Total number of cells in volume (V) = A , Percentage of
146 neutrophils in a sample (from flow cytometry) = X , Total number of Neutrophils in volume (V) =
147 $A.X$, Total enzyme in reaction volume = B (Interpolated from the standard curve). Total enzyme
148 per neutrophil = $B/(A.X)$

149

150 **Mathematical model**

151 A mechanistic mathematical model was developed based on existing knowledge of
152 granulopoiesis(13) and the following assumptions. Assumptions: (i) Differentiation of
153 granulocyte-monocyte progenitors (GMPs) to myelocytes occurs through several intermediate
154 stages (such as myeloblast and promyelocyte), with each stage having a specific proliferation rate.
155 The model assumes that the proliferating pool is kinetically homogeneous with identical turnover
156 rates for all the stages. (ii) The numbers of senescent neutrophils returning to bone marrow again
157 for clearance(16) are assumed to be negligible. (iii) Both in non-inflammatory and the induced
158 inflammatory condition, it is assumed that a steady-state is established, and the labeled cells are
159 tracked at the steady-state. (iv) As the half-life of EDU in circulation (around half an hour)(17) is
160 much lower than the timescale of the experiment, mitotic pool neutrophil progenitors/precursors
161 are assumed to be labeled instantaneously. Equations describing the percentage of EDU positive
162 neutrophils in various compartments:

163 **Proliferation pool**

$$\dot{X}_0 = -2.U.R.X_0$$

164 $\dot{X}_1 = 2.U.R.X_0 - 2.U.R.X_1$

⋮

$$\dot{X}_n = 2.U.R.X_{n-1} - 2.U.R.X_n$$

165 **Maturation pool**

$$\dot{Y}_1 = U.R.R_1 \sum_{i=0}^n X_i - s.Y_1$$

166 $\dot{Y}_2 = s.Y_1 - s.Y_2$

⋮

$$\dot{Y}_{h+1} = s.Y_h - s.Y_{h+1}$$

167 **Blood**

168 $\dot{B} = \frac{s}{R.R_1} Y_{h+1} - U.B$

169 **Peritoneum**

170 $\dot{P}e = w.(B - P e)$

171

172 **Observed bone marrow**

173 **data**

$$Y = \sum_{j=1}^{h+1} Y_j$$

174

175

176 The detailed derivation of the equations is provided in the Supplementary Information.

177

178 **Parameter estimation**

179 Agreement between model estimation and experimental data is quantified(18) as given below,

180 where noise in the experimental measurement is assumed to be normally distributed:

$$\chi^2 = \sum_{i=1}^n \sum_{j=1}^m \frac{Y_{i,j}(t) - Y_{i,j}}{\sigma^2}$$

181

X_i = percentage EDU⁺ cells that has undergone “i

“divisions

$$R = \frac{\text{number of neutrophils in blood at steady state}}{\text{number of neutrophils in the proliferation pool at steady state}}$$

n = number of divisions to EDU dilution

Y_j = percentage EDU⁺ maturing neutrophils cells in the

bone marrow compartments

$$R_1 = \frac{\text{number of neutrophils in the proliferation pool at steady state}}{\text{number of neutrophils in the maturation pool at steady state}}$$

s = egress rate from individual transit compartment

(1/hour)

h = number of transit compartments with transfer rate “s”

in maturation pool

B = percentage EDU⁺ neutrophils in blood

U = egress rate from blood (1/hour)

$P e$ = percentage EDU⁺ neutrophils in peritoneum

w = egress rate from peritoneum (1/hour)

182 n = number of datasets

183 m = number of time points

184 $Y_{i,j}$ = measured data

185 $Y_{i,j}(t)$ = estimated value

186

187 Equations are numerically solved using ODE45 in MATLAB with initial conditions that all
188 compartments except proliferation pool has no EdU tagged cells initially (at $t=0$). The initial
189 percentage of EDU tagged cells, α in the proliferation pool, is a parameter in the model. The
190 distribution of parameters yielding acceptable agreement between model and data are obtained
191 using iterative Approximate Bayesian Computation (iABC)(19) and iABC procedure was
192 implemented as described(20). SI and observability analysis were performed analytically (see
193 supplementary information).

194

195 **Statistics**

196 All data presented are based on at least 2 or more independent experiments with at least 3 animals
197 per experimental group. An independent experiment is described as an experiment involving
198 new/different batches of microspheres, mice and performed on a different date. Each 'n' represents
199 an individual animal. Data were analyzed, and graphs generated using GraphPad Prism 8
200 (GraphPad Software, La Jolla, CA, USA). One-way ANOVA was used for all statistical
201 comparisons involving multiple groups. For the neutrophil tracking data across different tissue
202 sites (BM, Blood and PC), one-way ANOVA was used at each time point. Significance is
203 represented as * $p<0.05$, ** $p<0.01$, *** $p<0.001$ and **** $p<0.0001$. Data are presented as mean
204 \pm standard deviation.

205

206 Common Language Effect Size (CLES) was used to determine statistical differences in parameters
207 estimated using the mathematical model. The CLES measure gives us the probability of one
208 random sample drawn from one distribution has a higher value than a randomly drawn sample

209 from another distribution. CLES measure was calculated using the MATLAB implementation(21)
210 and is reported with 95% confidence interval.
211

212 RESULTS

213 Biomaterial implant model for inducing inflammation

214 Mouse peritoneal cavity (PC) has been used as a model to study the molecular and cellular events
215 for initiation, persistence, and resolution of inflammation(22). Some of the most commonly used
216 irritants (zymosan, LPS and thioglycolate), however, result in an inflammatory microenvironment
217 that lasts for short (<3 days) periods(22–24). We have previously shown that peritoneal
218 implantation of sterile biomaterial microspheres results in sustained inflammation, which may be
219 used to study neutrophil production under inflammatory conditions(25). Hence, mice received
220 sterile biomaterial microspheres or saline as a control (referred to as mock). To tune the level of
221 inflammation, we used chitosan (highly stimulatory(26) in its crude form) and ultrapure alginate
222 (less stimulatory(14, 25)) to prepare the biomaterial microspheres (**Fig. S2**). Implantation of these
223 biomaterial microspheres resulted in recruitment of neutrophils to the implantation site for at least
224 ten days, with a concomitant increase in the percentage of these cells (**Fig. S3**), as reported
225 previously(14, 25).

226

227 As a measure of the level of inflammation, we determine the proportions of granulocyte-monocyte
228 progenitors (GMP), which increase when an inflammatory stimulus induces emergency
229 granulopoiesis(27). GMP population was identified as Lineage⁻ c-Kit⁺ Sca-1⁻ CD16/32⁺ CD34⁺
230 cells through flow cytometry (**Fig. S4**). We observe that in mice implanted with alginate
231 microspheres, the percentages (and number) of granulocyte-monocyte progenitors (GMP) in both
232 the bone marrow and spleen were similar to those in mock controls at seven- and ten-day post-
233 implantation (**Fig. 1A**). In contrast, chitosan microsphere implantation significantly increased
234 GMP percentages in bone marrow and spleen (**Fig. 1A**).

235

236 To further understand the effects of microsphere implantation, we studied the phenotype and
237 granular content of neutrophils isolated from bone marrow, blood and PC (implant site). For
238 phenotyping, we measured the surface expression levels of CD11b, ICAM-1, CD62L and CXCR2
239 on neutrophils at seven- and ten-day post-implantation. The expression levels of these proteins are
240 expected to vary based on the level of cellular activation(28). We observed that in neutrophils
241 retrieved from the bone marrow and blood of mice implanted with chitosan microspheres,

242 expression of CD11b and ICAM-1 following *ex vivo* activation is significantly lower compared to
243 cells from mice implanted with alginate microspheres or mock controls (**Fig. 1B and 1C**). These
244 differences are not observed among neutrophils at the site of inflammation (**Fig. 1D**). Additionally,
245 activation-dependent upregulation of CD11b and ICAM-1 expression was significantly reduced
246 among neutrophils from mice implanted with chitosan microspheres (**Fig. S5**). Activation-
247 dependent downregulation of CD62L and CXCR2 expression was also compromised in
248 neutrophils isolated from the blood of mice implanted with chitosan microspheres as compared to
249 those from mice with alginate microspheres or mock controls (**Fig. S6**). The granular content of
250 neutrophils from the blood of mice implanted with microspheres was also different relative to
251 mock controls. Significantly lower amounts of myeloperoxidase (MPO) and elastase per
252 neutrophil were observed in the blood of mice with microsphere implants (**Fig. 1E**).

253

254 Overall, increased GMP percentage in the bone marrow and spleen, and altered surface protein
255 expression and reduced granule enzyme content among neutrophils in circulation suggest that
256 emergency granulopoiesis (EG)-like conditions are induced following chitosan microsphere
257 implantation. However, as GMP levels remains similar in mice with alginate microspheres and
258 mock controls, we label the former as having caused inflammation but not inducing emergency
259 granulopoiesis.

260

261 **Neutrophil Kinetics**

262 We next assessed the kinetics of neutrophils under non-inflammatory (mock), inflammatory-
263 (alginate), and inflammation-inducing EG-like (chitosan) conditions. 5-ethynyl-2-deoxyuridine
264 (EdU) labeled neutrophils were identified through the gating strategy described in **Fig. 2A**. Under
265 non-inflammatory and inflammatory (but not EG-like) conditions, labeled neutrophil peaks were
266 observed at day E2 in bone marrow and day E3-E4 in the blood, which is line with recently
267 published data on neutrophils kinetics under steady-state conditions(6). In the presence of
268 inflammation that induces EG-like conditions, we observed that labeled neutrophils appeared
269 earlier in the bone marrow (at day E1, **Fig. 2B**) and blood (at day E2, **Fig. 2C**) as compared to the
270 other two conditions. Percentages of labeled neutrophils in the PC (**Fig. 2D**) followed a trend
271 similar to those in circulation. Under EG-like conditions, the peak of labeled neutrophils appeared

272 at day E2-E3, which was earlier than the peak observed in the other two conditions (day E3-E4).
273 The differences in the timing of the peak of labeled neutrophils at each tissue site in the mice with
274 EG-like conditions suggest a faster release of neutrophils into the circulation and early arrival of
275 these labeled cells at the inflammatory site.

276

277 Basu et al.(12) previously described differences in neutrophil kinetics based on the extent of stain
278 incorporation. We analyzed our data similarly by separating the EdU incorporated neutrophils as
279 either high expression of EdU (neutrophil incorporating EdU in their last stages of division) or
280 medium expression of EdU (neutrophils that have undergone few divisions after EdU
281 incorporation). Similar to the observations from total EdU-labeled cells, EdU-high and EdU-
282 medium cells appeared earlier in the blood and PC of mice implanted with chitosan microspheres,
283 compared to other conditions (**Fig. S7**). Additionally, we observed a one-day delay in EdU-
284 medium cells' peaks compared to EdU-high cells in all groups. This delay is expected as the latter
285 are cells arising from progenitors in their last stages of division, leading to a faster appearance in
286 the maturation pool and circulation(12).

287

288 The overall time taken for labeled neutrophils to appear and then disappear may also be analyzed
289 to provide insights into residence time in various compartments. One method often employed to
290 understand half-life and residence times is fitting an exponential decay curve from the peak(6, 12).
291 However, an exponential decay function is not an actual depiction of the underlying process and
292 may lead to inaccurate estimation of the parameters. Therefore, we developed a mechanistic model
293 to extract kinetic parameters from the experimental data.

294

295 **Quantifying Kinetic Parameters**

296 We applied a system of differential equations that explicitly model EDU dilution, neutrophil
297 maturation in the bone marrow, and residence times in the blood and tissue (**Fig. S8**). The model
298 parameters must be Structurally Identifiable (which is a consequence of the model topology) for
299 them to be estimated(29, 30). By analyzing the transfer functions of the experimentally observed
300 variables and the observability of internal state variables, we determine that the model parameters
301 were identifiable (supplementary information). Then, we fit the model to the data obtained from

302 mock controls and microsphere implanted mice, beginning with uniform priors for all the
303 parameters in iterative Approximate Bayesian Computation (iABC). Representative fits (~1000)
304 of the model to data (**Fig. 3**) and the overall distribution of each parameter (25000 parameter sets
305 under acceptable chi-square cut-off) are shown (**Fig. 4**).

306

307 The practical identifiability of the parameter (which depends on the discrete nature and quality of
308 the measured data) appears as the magnitude of spread in the parameter distributions(31, 32). This
309 spread is presented in **Table 1** as the medians and 95% confidence intervals of each parameter.
310 Using these parameters, we calculated the values for maturation time in the bone marrow, and half-
311 life and residence time in the blood and PC (**Table 2**). Owing to the large sample size in parameter
312 distributions, comparing the distributions between different groups will show statistical
313 significance even if the differences are very small. To look at practical significance of the
314 differences, which would not be greatly influenced by the large sample size, a non-parametric
315 effect size measure (Common Language Effect Size (CLES)), was used to quantify the
316 differences(33). CLES was calculated between different groups for all the parameters and
317 tabulated (**Table S2**).

318

319 Through these steps, we determined that in mice with inflammation that induces EG-like
320 conditions, the neutrophil maturation time in the bone marrow is considerably lower compared to
321 the other two conditions. While this was apparent from the experimental data shown in Fig. 2 (peak
322 of EdU labelled neutrophils in blood appearing at day 2 in mice with chitosan microspheres), the
323 mathematical model allowed us determine that the median of the range of maturation times was
324 lowered to 26 hours (compared to the expected 40 hours under non-inflammatory conditions).
325 Additionally, we observed that half-life (and consequently residence time) in blood decreased,
326 while half-life in PC increased by two-fold in mice with EG-like conditions compared to non-
327 inflammatory conditions. This was, in fact, not apparent from the experimental data.

328

329 Together, these data suggest that in response to inflammation resulting in EG-like conditions,
330 neutrophils are generated and released faster from the bone marrow and spend less time in the

331 blood and more time at the site of inflammation when compared to a non-inflammatory condition.
332 In contrast, under a milder inflammatory condition (alginate implants), maturation time is not
333 altered, but the half-life of neutrophils in the blood increases modestly.

334 **DISCUSSION**

335 Neutrophils play an essential role in pathogen and foreign body clearance(34). However, their
336 aberrant activity may result in pathological conditions such as inflammatory bowel disease(35),
337 rheumatoid arthritis(36), and acute respiratory distress syndrome(37). A potential strategy to
338 enable their beneficial roles while also limiting their damaging effects is the modulation of
339 neutrophil frequencies and life cycle(1, 13, 38). To achieve such modulation, we must first
340 determine neutrophil kinetics under inflammatory conditions.

341

342 Granulopoiesis under emergency conditions has been explored by injecting granulocyte colony
343 stimulating factor (G-CSF)(11) or *E. coli*(39). Both G-CSF and *E. coli* injections resulted in
344 neutrophils appearing faster in circulation (11, 39), and it was suggested (but not demonstrated)
345 that this was due to reduced maturation time in the bone marrow. Another study has determined
346 changes in neutrophil production rates in the bone marrow following a burn injury(40), but other
347 aspects of the kinetics have not been determined. Our data on neutrophil kinetics under emergency
348 granulopoiesis-like conditions induced by chitosan microspheres is in agreement with these
349 reports, and demonstrates that maturation time in the bone marrow is indeed reduced. Alterations
350 in maturation time could have implications on neutrophil phenotype and functions. For example,
351 the lowered capacity to upregulate activation markers (such as CD11b) and lower granule protein
352 content per cell could be a consequence of reduced maturation times in mice implanted with
353 chitosan microspheres. We also determine neutrophils kinetics under conditions that induce
354 inflammation but do not appear to cause emergency granulopoiesis (alginate microsphere
355 implantation). Under such conditions, neutrophil maturation times in the bone marrow remain
356 unchanged.

357

358 Further, no previous report describes neutrophil kinetics at the site of inflammation. In this context,
359 a recent study by Ballesteros et al.(6) shows that neutrophil half-life in different tissues under
360 steady-state conditions is similar (except in skin) to their half-life in the blood. It has also been
361 suggested that inflammation may extend neutrophils' lifespan at the inflammatory tissue site(2, 41,
362 42). Our data show an increase in half-life (and consequently lifespan) of neutrophils at a sterile
363 inflammatory site if the inflammation induces EG-like conditions.

364

365 To estimate maturation times and lifespans of neutrophils in various tissues, we have developed a
366 new model to fit the data. Prior studies have fit an exponential decay function (peak to baseline)
367 to similar experimental data(6, 11, 12), but such modeling ignores the simultaneous ingress of
368 labeled cells during that period resulting in over-estimation of half-lives. Additionally, deriving
369 information on specific aspects of kinetics, such as maturation times in the bone marrow, is not
370 possible using exponential decay based fitting methods. Hence, we modeled the process of
371 granulopoiesis and neutrophil presence in tissues mechanistically, to extract kinetic parameters
372 with an acceptable spread in distributions. Our model provided quantifiable values for most
373 parameters, except for the peritoneal egress rate from mice implanted with alginate microspheres.
374 This could be because of the large variability seen in the experimental data in this group.

375

376 One caveat to the data and the model presented here are that we assume that the number of reverse-
377 migrating neutrophils(43) in the bone marrow is negligible compared to the numbers present in
378 the maturation compartment. Another shortcoming is that we do not explicitly include the
379 marginated pool of neutrophils present in the lungs and liver. A logical next step to the current
380 study would be to determine how both reverse migration and marginated pool of neutrophils are
381 altered under inflammatory conditions.

382

383 Results presented here showcases the possibility of using biomaterials as a tool to study immune
384 cell dynamics(44, 45). Biomaterials induce differing grades of immune responses based on the
385 chemical nature of the material used and on the physical (shape, size, morphology etc.)
386 characteristics of the implant(46, 47). An example of this variation is demonstrated here with
387 alginate and chitosan-based biomaterial implants. While the chemical composition of these
388 materials is dissimilar and the purity of the base material was different, the exact reasons that these
389 materials induce distinct immune responses remains unclear. Nevertheless, it is noteworthy that
390 the implantation of biomaterials (specifically, chitosan) in the peritoneal cavity results in a
391 dramatic change in neutrophil kinetics, which could have implications in our methodologies to test
392 the compatibility of materials for *in vivo* use.

393

394 In conclusion, we show that in the presence of inflammation that induces EG-like conditions,
395 neutrophil maturation time in the bone marrow and half-life in the blood reduces, and residence
396 time at the inflammatory site increases when compared to non-inflammatory and low-grade
397 inflammatory stimuli. The functional impact of such changes remain to be evaluated.

398

399

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403

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FIGURES

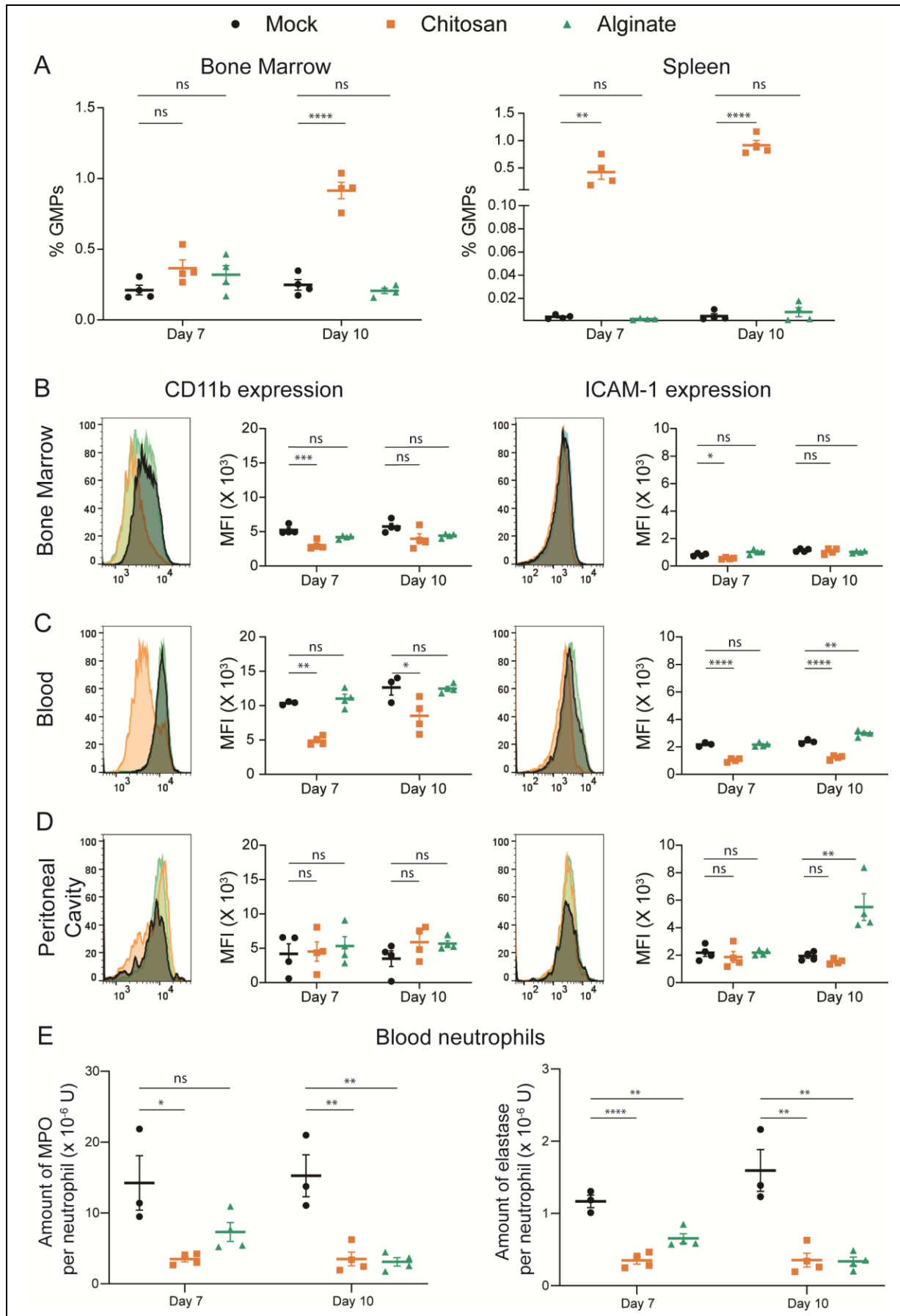


Figure 1. Progenitor numbers and neutrophil phenotype post implantation of sterile biomaterial microspheres. **A** – Quantification of granulocyte-monocyte progenitors (GMPs) as a percentage of total live single cells from bone marrow (BM) and spleen at day 7 and 10 after mock or microsphere-implantation procedure. **B-D** – Phenotype of neutrophils at different tissues, at day 7 and 10 after mock or microsphere-implantation procedure. CD11b and ICAM-1 expression levels among neutrophils following ex vivo activation in BM (**B**), blood (**C**) and peritoneal cavity (**D**). **E** – Total intracellular MPO and elastase content per neutrophil in the blood. Saline and chitosan group is representative of 2 independent experiments with total n = 4 mice per group. Alginate group is representative of 1 independent experiment with n = 4 mice at each time point, involving both male and female mice. For statistical analyses, a one-way ANOVA was performed followed by Tukey post-test, and * = p < 0.05; ** = p < 0.01; *** = p < 0.001; and **** = p < 0.0001.

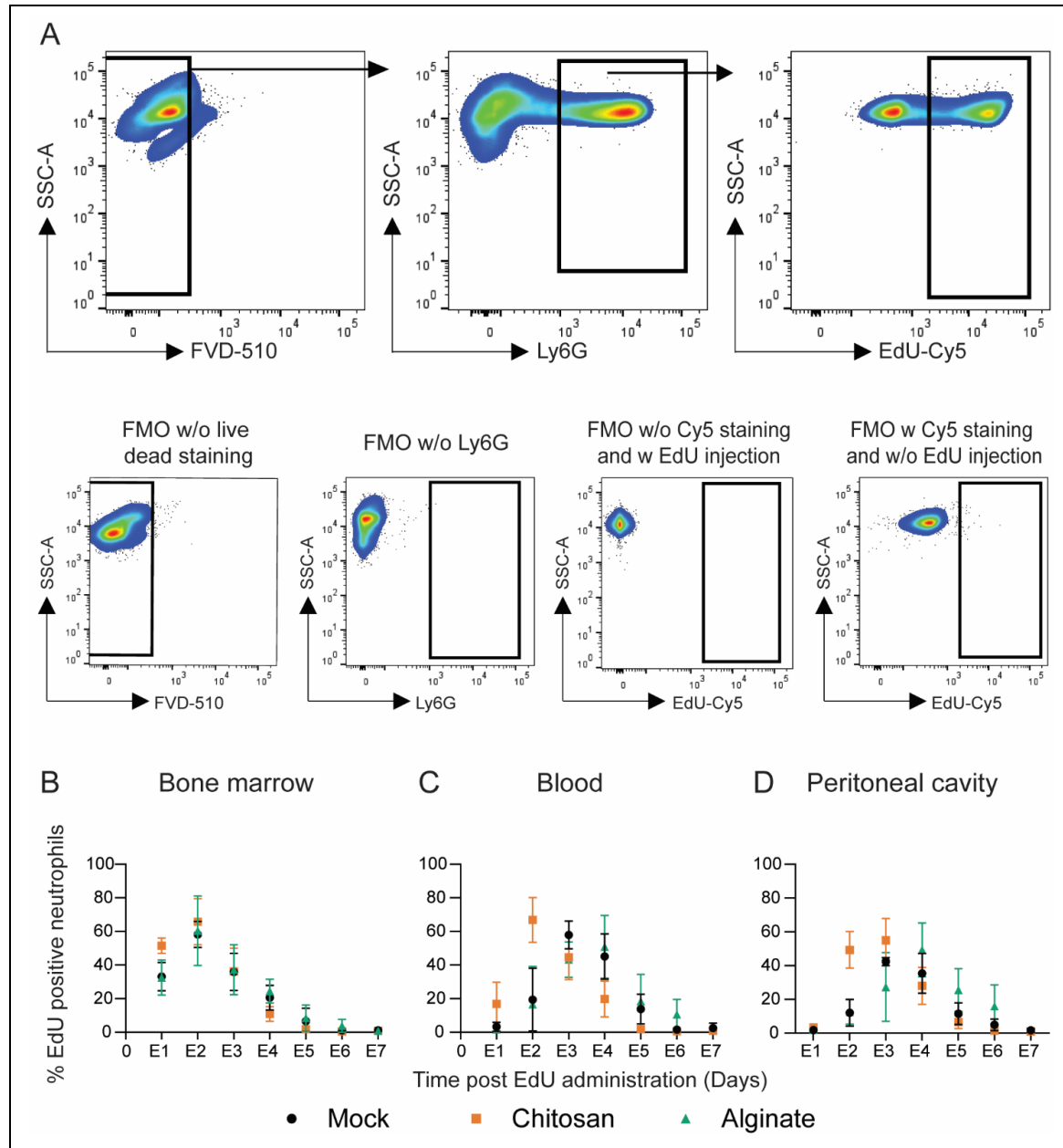


Figure 2. *In vivo* tracking of labeled neutrophils. **A** - Gating strategy used to determine labeled neutrophils. Fluorescence-minus-one (FMO) plots were used to ascertain gate positions. Plots are representative of multiple independent experiments. **B-D** – Labeled neutrophil (EdU positive) percentages in bone marrow (**B**) blood (**C**) and peritoneal cavity (**D**) at different times. N = 3-7 mice/time point/per group pooled from at least 3 independent experiments including both male and female mice. For statistical analyses, at each time point, a one-way ANOVA was performed followed by Tukey post-test. Statistical analysis is summarized in **Table S1**.

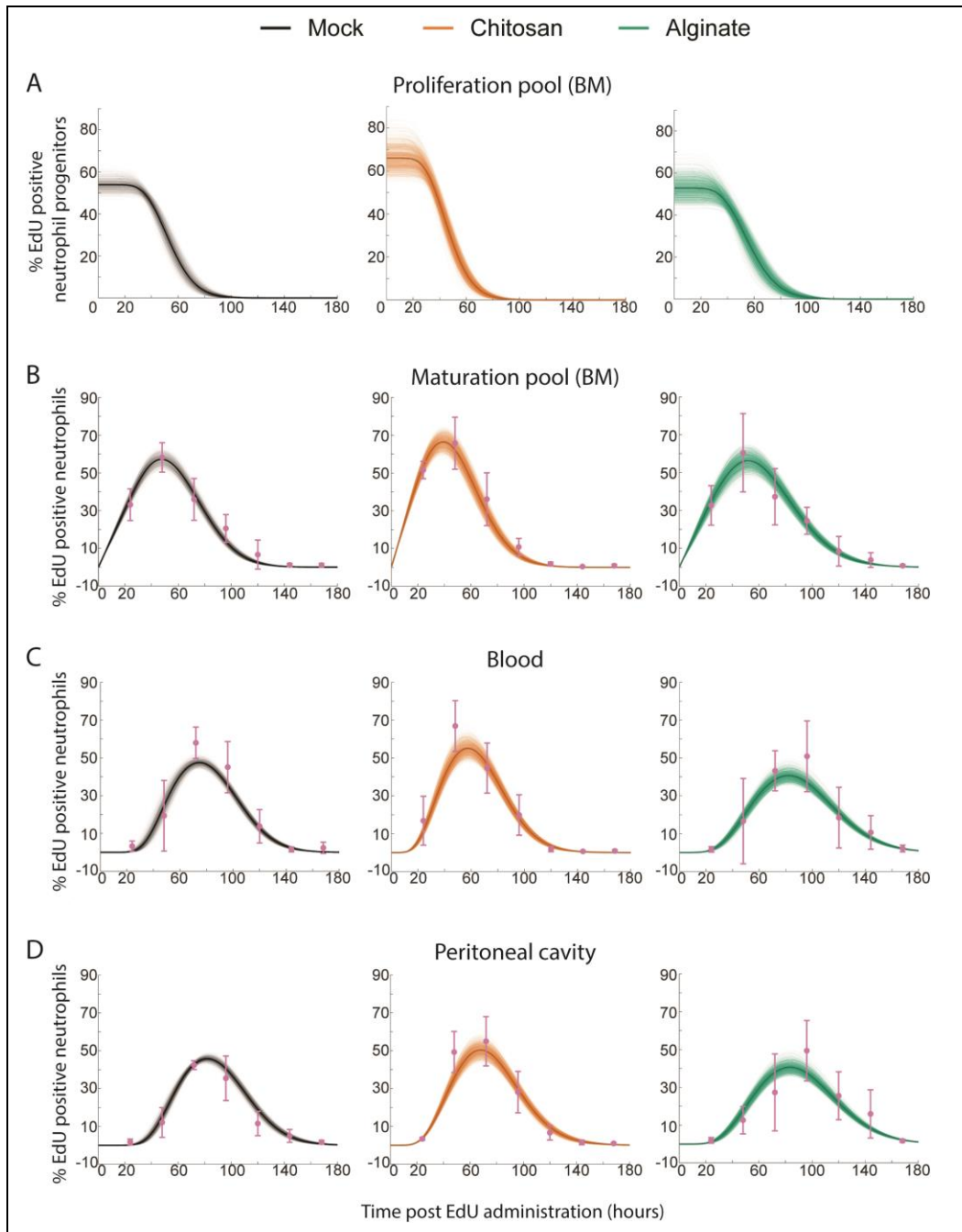


Figure 3. Fitting the mathematical model to experimental data. Representative fits to mock, chitosan and alginate data. Sample curves corresponding to different parameters sets in proliferation pool (A), maturation pool (B), blood (C) and peritoneal cavity (D) are shown as thin lines and average is shown as thick solid line. Experimentally measured data are shown as pink dots with standard deviation

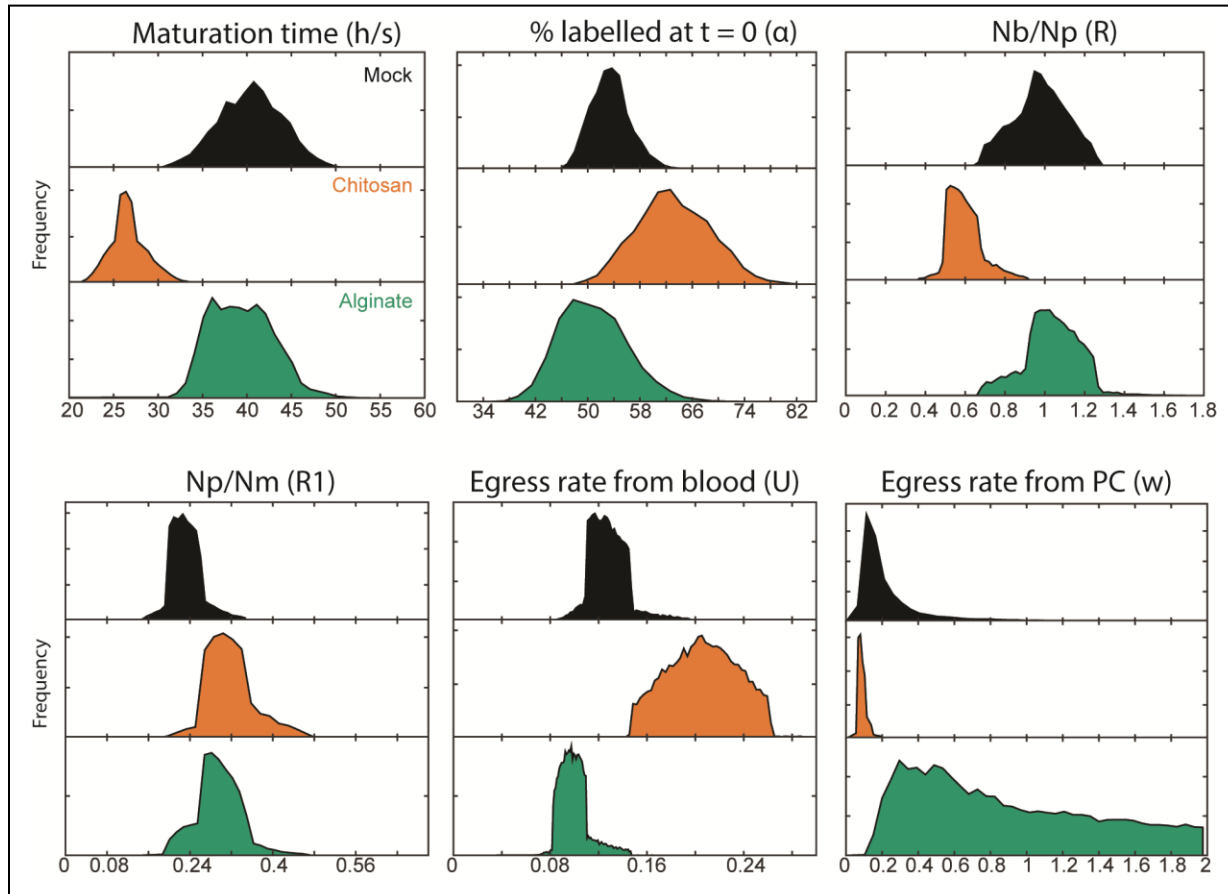


Figure 4. - Distributions of parameters obtained from the model. At the end of final iteration of iABC, the possible numerical values for each parameter are provided as a frequency distribution. N_p – Number of neutrophils in the proliferation pool at steady state, N_b – Number of neutrophils in the blood at steady state, N_m – Number of neutrophils in the maturation pool at steady state.

| | Mock | | | Chitosan | | | Alginate | | |
|-------------------------------------------------------------------------------------------------------|--------------|-------|-------|--------------|-------|-------|--------------|-------|-------|
| | median | ci | | median | ci | | median | ci | |
| n (number of divisions to EDU dilution) | 12 | 10 | 16 | 10 | 8 | 14 | 11 | 8 | 14 |
| α (initial percentage of labelled cells) | 53.37 | 48.16 | 60.13 | 62.84 | 52.53 | 75.28 | 50.43 | 41.95 | 61.88 |
| U (hour⁻¹) (egress rate from blood) | 0.12 | 0.10 | 0.16 | 0.20 | 0.15 | 0.25 | 0.09 | 0.08 | 0.13 |
| R (Number of neutrophils in blood / Number of neutrophils in proliferation pool) | 0.97 | 0.70 | 1.23 | 0.58 | 0.46 | 0.83 | 1.03 | 0.73 | 1.25 |
| R1 (Number of neutrophils in proliferation pool / Number of neutrophils in maturation pool) | 0.23 | 0.17 | 0.31 | 0.31 | 0.240 | 0.43 | 0.29 | 0.20 | 0.39 |
| s (hour⁻¹) (egress rate from individual transit compartment) | 0.29 | 0.23 | 0.34 | 0.16 | 0.14 | 0.19 | 0.12 | 0.10 | 0.16 |
| h (number of transit compartment with transfer rate “s” in maturation pool) | 12 | 9 | 15 | 5 | 4 | 5 | 5 | 4 | 6 |
| w (hour⁻¹) (egress rate from peritoneum) | 0.17 | 0.08 | 1.41 | 0.08 | 0.06 | 0.16 | 0.77 | 0.20 | 1.91 |

Table 1 - Rate parameters estimated from the mathematical model. Median and 95% confidence interval (ci) of the possible values the parameters can take based on our numerical simulation are tabulated.

| | Mock | | | Chitosan | | | Alginate | | |
|---------------------------------------------------------|--------------|-------|-------|--------------|-------|-------|--------------|-------|-------|
| | median | ci | | median | ci | | median | ci | |
| Maturation time in bone marrow (h/s) (hours) | 40.50 | 33.27 | 47.40 | 26.50 | 22.87 | 31.34 | 39.23 | 33.82 | 46.55 |
| Half-life in blood (ln(2)/U) (hours) | 5.46 | 4.089 | 6.81 | 3.35 | 2.67 | 4.55 | 7.04 | 5.14 | 8.36 |
| Residence time in blood (1/U) (hours) | 7.88 | 5.89 | 9.83 | 4.84 | 3.85 | 6.57 | 10.17 | 7.42 | 12.06 |
| Half-life in peritoneum (ln(2)/w) (hours) | 3.99 | 0.49 | 8.10 | 8.05 | 4.10 | 11.03 | 0.89 | 0.36 | 3.38 |
| Residence time in peritoneum (1/w) (hours) | 5.76 | 0.70 | 11.69 | 11.61 | 5.91 | 15.92 | 1.29 | 0.52 | 4.87 |

Table 2 - Calculated parameters of neutrophil kinetics. From the rate parameters presented in table 1, parameters of interest were calculated and are presented here as median and 95% confidence interval (ci) of the possible values the parameters can take.