

1 **Bisphenol S and bisphenol F are less disruptive to cardiac electrophysiology and**
2 **potentially safer for use in medical products, as compared to bisphenol A**

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28 **Conflict of interest:** None.

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34 **ABSTRACT**

35 **Background:** Bisphenol A (BPA) is a high-production volume chemical that is commonly used to
36 manufacture consumer and medical-grade plastic products. Due to its ubiquity, the general
37 population can incur daily environmental exposure to BPA, while heightened BPA exposure has
38 been reported in intensive care patients and industrial workers. Due to health concerns,
39 structural analogues are being explored as replacements for BPA.

40 **Objective:** This study aimed to examine the direct nongenomic effects of BPA on cardiac
41 electrophysiology and compare its safety profile to recently developed alternatives, including
42 BPS (bisphenol S) and BPF (bisphenol F).

43 **Methods:** Whole-cell voltage-clamp recordings were performed on cell lines transfected with
44 Nav1.5, hERG, or Cav1.2. Results of single channel experiments were validated by conducting
45 electrophysiology studies on human induced pluripotent stem cell-derived cardiomyocytes
46 (hiPSC-CM) and intact, whole heart preparations.

47 **Results:** Of the chemicals tested, BPA was the most potent inhibitor of both fast (I_{Na-P}) and late
48 (I_{Na-L}) sodium channel ($IC_{50} = 55.3$ and $23.6 \mu M$, respectively), L-type calcium channel ($IC_{50} =$
49 $30.8 \mu M$) and hERG channel current ($IC_{50} = 127 \mu M$). The inhibitory effects of BPA and BPF on
50 L-type calcium channels were supported by microelectrode array recordings, which revealed
51 shortening of the extracellular field potential (akin to QT interval). Further, BPA and BPF
52 exposure impaired atrioventricular conduction in intact, whole heart experiments. BPS did not
53 alter any of the cardiac electrophysiology parameters tested.

54 **Discussion:** Results of this study demonstrate that BPA and BPF exert an immediate inhibitory
55 effect on cardiac ion channels, and that BPS may be a safer alternative. Intracellular signaling
56 or genomic effects of bisphenol analogues were not investigated; therefore, additional
57 mechanistic studies are necessary to fully elucidate the safety profile of bisphenol analogues on
58 the heart.

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60

61 **INTRODUCTION**

62 Bisphenol A (BPA) is a high production volume chemical, with roughly 8 million metric tons used
63 each year to manufacture polycarbonate plastics (e.g., food and beverage containers, medical
64 devices), epoxy resins (e.g., aluminum can liners), and in thermal printing applications (PR
65 newswire 2016; Shelby 2008). Human exposure to BPA can occur daily, and as a result,
66 biomonitoring studies have detected BPA in 91-99% of the general population (Calafat et al.
67 2005; Chen et al. 2016a; Lehmler et al. 2018; Vandenberg et al. 2007, 2010). Although
68 environmental exposure to BPA occurs at a relatively low dose (Koch and Calafat 2009;
69 Vandenberg et al. 2007, 2010), occupational (Hines et al. 2018; Ribeiro et al. 2017) and clinical
70 environments can result in exceedingly high BPA exposure (Calafat et al. 2009; Duty et al.
71 2013; Gaynor et al. 2018; Huygh et al. 2015; Testai et al. 2016). Indeed, BPA was detected in
72 60% of neonatal intensive care unit (NICU) supplies, including items used for feeding,
73 bandages, breathing support, intravenous and parenteral infusion (Iribarne-Durán et al. 2019).
74 Clinical exposure can also result in heightened and/or prolonged BPA exposure in young
75 patients, due to an underdeveloped metabolic system (Calafat et al. 2009). In the NICU setting,
76 premature infants had urinary BPA levels that ranged from 1.6–946 µg/L (Calafat et al. 2009)
77 and the degree of exposure was linked to high-intensity treatment that required multiple (plastic)
78 medical devices (Duty et al. 2013). Similarly, adult ICU patients were found to have urinary BPA
79 levels that ranged from 6.1–680 µg/L when undergoing extracorporeal membrane oxygenation
80 in conjunction with continuous vevo-venous hemofiltration (Huygh et al. 2015).

81
82 BPA exposure is concerning, particularly in sensitive patient populations, as accumulating
83 evidence suggests that BPA exerts a negative impact on cardiovascular health (Bae et al. 2012;
84 Bae and Hong 2015; Han and Hong 2016; Melzer et al. 2010, 2012). A 10-year longitudinal
85 study found that BPA exposure was associated with a 46-49% higher hazard ratio for
86 cardiovascular and all-cause mortality (Bao et al. 2020). Further, epidemiological studies have
87 reported associations between BPA exposure and an increased risk of myocardial infarction,
88 hypertension, coronary and peripheral artery disease, and a decrease in heart rate variability
89 (reviewed previously (Posnack 2014; Ramadan et al. 2020). Experimental studies have noted
90 that BPA exposure can antagonize ion channels, impair electrical conduction, and precipitate
91 triggered arrhythmias (Belcher et al. 2011; Deutschmann et al. 2013; Feiteiro et al. 2018;
92 Michaela et al. 2014; Posnack et al. 2015; Wang et al. 2011; Yan et al. 2011). *In vitro* studies
93 performed in HEK, neuronal, and smooth muscle cells have shown that BPA inhibits T-type and
94 L-type calcium channel current (Deutschmann et al. 2013; Feiteiro et al. 2018; Michaela et al.

95 2014). In cardiac tissue, such an alteration in calcium channel current would alter nodal cell
96 depolarization, atrioventricular conduction, and the plateau phase of the cardiac action potential.
97 Further, BPA exposure can disrupt intracellular calcium handling, resulting in calcium leak from
98 the sarcoplasmic reticulum and an increased propensity for triggered arrhythmias (Gao et al.
99 2013; Liang et al. 2014; Ramadan et al. 2018). Of interest, BPA exposure was observed to
100 increase calcium-mediated triggered activity and ventricular arrhythmias in females (but not
101 males) that were subjected to catecholamine stress. Notably, such alterations in calcium
102 handling were attenuated in an estrogen-receptor knockout model (Yan et al. 2011), which
103 supports the claim that BPA-induced effects are sex specific.

104
105 With increasing health concerns, structurally similar chemicals are being explored as
106 replacements for BPA (Chen et al. 2016a). Two such substitutes, bisphenol S (BPS) and
107 bisphenol F (BPF), are used to manufacture consumer products that don 'BPA-free' labeling.
108 For example, BPS is used to produce polyethersulfone plastic food containers, medical-grade
109 products, epoxy resins, and is found in thermal printing applications (Chen et al. 2016a; Lehmler
110 et al. 2018). Unfortunately, many of these alternative chemicals are considered 'regrettable
111 substitutions', as BPS and BPF may exert biological effects that are similar to BPA (Kojima et al.
112 2019; Moon 2019; Trasande 2017). To date, it is unclear whether BPA alternatives offer a
113 superior cardiac safety profile, as recent work suggests that BPS and BPF may also impair
114 cardiac function (Ferguson et al. 2019; Gao et al. 2015; Mu et al. 2019). Recent biomonitoring
115 studies have observed an uptick in BPS and BPF exposure in the general population as BPA is
116 phased out and replaced (Lehmler et al. 2018), which highlights the urgent need to investigate
117 the impact of BPA analogues on cardiac health.

118
119 We compared the cardiac safety profile of BPA, BPS, and BPF using whole-cell voltage clamp
120 experiments to identify the half maximal inhibitory concentration (IC_{50}) of four key cardiac ion
121 channels, highlighted by the CiPA (comprehensive in vitro proarrhythmia) initiative (Colatsky et
122 al. 2016; Sager et al. 2014). The results of single channel experiments were validated by
123 conducting electrophysiology studies on human induced pluripotent stem cell-derived
124 cardiomyocytes (hiPSC-CM) using microelectrode array (MEA) recordings. Importantly, hiPSC-
125 CM have been widely adopted as a tool for preclinical safety testing to measure alterations in
126 cardiac automaticity, conduction velocity, depolarization, and repolarization time (Chen et al.
127 2016b). To aid in the translation of our *in vitro* cell studies, we employed an intact, whole heart
128 preparation for direct assessment of cardiac electrophysiology. We hypothesized that inhibitory

129 effects of bisphenol chemicals on calcium current would present with delayed atrioventricular
130 conduction in cardiac preparations. Further, we hypothesized that BPS and/or BPF exposure
131 would have less effect on cardiac electrophysiology, due to differences in chemical structure
132 that may increase the potency of BPA for voltage-gated channels (Deutschmann et al. 2013).

133

134 **METHODS**

135 Reagents

136 Bisphenol A (CAS #80-05-7), bisphenol S (CAS #80-09-1), and bisphenol F (CAS #620-92-8)
137 were purchased from Sigma Aldrich ($\geq 98\%$ purity, analytical standard). Stock solutions of BPA,
138 BPS, or BPF were prepared in 99+% dimethyl sulfoxide (DMSO), and working concentrations
139 were prepared directly in cell culture media (voltage-clamp recordings, MEA studies) or Krebs-
140 Henseleit (KH) crystalloid buffer (intact heart preparations) to obtain a final concentration
141 between 0.01-100 μM BPA, BPS, or BPF. This range of doses was selected to mimic
142 environmental, clinical, and supraphysiological exposure levels (Ramadan et al. 2018).

143

144 Whole-cell voltage-clamp recordings

145 Nav1.5, Cav1.2, and hERG channel recordings were performed at room temperature (25°C)
146 using stably transfected cell lines, as previously described (Jaimes et al. 2019). For Nav1.5
147 recordings, the extracellular solution included 137 mM NaCl, 10 mM dextrose, 10 mM HEPES, 4
148 mM KCl, 1 mM MgCl_2 , and 1 mM CaCl_2 . The intracellular solution consisted of 120 mM CsOH,
149 120 mM aspartic acid, 10 mM EGTA, 10 mM CsCl, 10 mM HEPES, 5 MgATP, and 0.4 mM Tris-
150 GTP. The voltage protocol was approximately 1 sec in duration, repeated at 0.1 Hz. Sodium
151 channel recordings were performed using HEK293 cells transfected with Nav1.5 cDNA. Cells
152 were repolarized from -95 to -120 mV for 200 msec, depolarized from -120 to -15 mV for 40
153 msec, and then further depolarized to +40 mV for 200 msec. This was followed immediately by
154 a voltage ramp down phase from +40 to -95 mV for 100 msec. ATXII (20 nmol/L) was included
155 in the extracellular solution to induce Nav1.5 late current, as previously described (Mantegazza
156 et al. 1998). Tetrodotoxin (30 μM) was applied at the end of each recording to determine the
157 current baseline. Cav1.2 recordings were performed using CHO cells stably transfected with
158 Cav1.2 cDNA. Cells were depolarized from -80 mV to 0 mV for 40 msec, further depolarized to
159 +30 mV for 200 msec, followed by a voltage ramp down phase from +30 mV to -80 mV for 100
160 msec. Recording stability was assessed by applying the voltage protocol in control solution for
161 12 consecutively recorded traces with <10% difference. hERG recordings were performed using
162 HEK293 cells stably transfected with hERG cDNA. The extracellular solution included 130 mM

163 NaCl, 12.5 mM dextrose, 10 mM HEPES, 5 mM KCl, 1 mM MgCl₂:6H₂O, and 1 mM CaCl₂. The
164 intracellular solution consisted of 120 K-gluconate, 20 mM KCl, 10 mM HEPES, 5 EGTA, and
165 1.5 MgATP. The voltage protocol was 5 sec in duration, repeated at 0.1 Hz. Cells were
166 depolarized -80 mV to +40 mV for 500 msec, followed by a voltage ramp down phase from +40
167 mV to -80 mV for 100 msec. A hERG potassium channel blocker (10 μM E-4031) was applied at
168 the end of each recording to determine the baseline. Recordings were collected before and after
169 bisphenol chemical exposure; chemical potency was calculated by dividing the steady state
170 current amplitude by the average amplitude from the last 5 traces measured in control solution
171 to calculate the fractional block. This was plotted against the bisphenol chemical concentration
172 tested, fitted with the Hill Equation to generate a half-maximal inhibitory concentration (IC₅₀) and
173 the Hill coefficient.

174

175 Human cardiomyocyte microelectrode array recordings

176 hiPSC-CM (iCell cardiomyocytes², female donor #01434, Fujifilm) were plated onto fibronectin-
177 coated microelectrode arrays at a density of 50-75,000 cells/well (24-well plate, Axion). Cells
178 were defrosted in iCell cardiomyocyte plating media in a cell culture incubator (37°C, 5% CO₂)
179 for 2 hours, thereafter cells were cultured in iCell maintenance media for the duration of study.
180 Treatment groups included 0.01% DMSO (vehicle), 0.01-100 μM BPA, BPS, or BPF. Cells were
181 treated for 15 minutes, and then extracellular field potential signals were recorded in response
182 to external stimulation (1-2 Hz). Extracellular field potential duration (FPD) was measured and
183 rate corrected with Frederica formula (FPDc). Disturbances in the recorded waveform can be
184 used to predict the identity of ion channels impacted by chemical exposure, with FPD analogous
185 to an *in vitro* QT interval that correlates with action potential duration at 50% repolarization
186 (Asakura et al.; Clements 2016).

187

188 Animals

189 Animal protocols were approved by the Institutional Animal Care and Use Committee at
190 Children's National Research Institute and followed the National Institutes of Health's *Guide for*
191 *the Care and Use of Laboratory Animals*. Bisphenol chemicals are xenoestrogens that may
192 cause exaggerated cardiac effects in females (Ben-Jonathan and Steinmetz 1998; Yan et al.
193 2011); accordingly, experiments were performed using female Sprague-Dawley rats, aged 3-4
194 months (Taconic Biosciences, strain NTac:SD, from NIH Genetic Resource stock, n=66).
195 Animals were housed in conventional acrylic rat cages in the Research Animal Facility, under
196 standard environmental conditions (12:12 hour light:dark cycle, 18–25°C, 30-70% humidity).

197 Each animal served as its own control, with electrophysiology measurements collected at
198 baseline and again after treatment.

199

200 Intact heart preparations

201 Animals were anesthetized with 3% isoflurane; the chest was opened, the heart was rapidly
202 excised, and the aorta was cannulated. The isolated, intact heart was then transferred to a
203 temperature-controlled (37°C) constant-pressure (70 mmHg) Langendorff-perfusion system.
204 Excised hearts were perfused with a modified Krebs-Henseleit buffer bubbled with carbogen, as
205 previously described (Jaimes et al. 2019). Pseudo-electrocardiograms (ECG) were recorded in
206 lead II configuration, and biosignals were acquired in iox2 and analyzed in ecgAUTO. Isolated
207 hearts remained stable with minimal fluctuations in heart rate or electrophysiology parameters
208 following 0.01% DMSO media perfusion (vehicle; **Figure 1**). To account for animal variability,
209 ECG recordings were collected throughout the study, during control media perfusion (15 min)
210 and in response to bisphenol chemical exposure (15 min). Similarly, electrophysiology
211 measurements (see below) were measured at baseline, after 15 min chemical exposure, and
212 again after 15 min washout with KH media.

213

214 Electrophysiology measurements

215 A pacing electrode was positioned on the right atrium for assessment of atrioventricular (AV)
216 conduction time, AV node refractory period (AVNERP) and Wenckebach cycle length (WBCL).
217 WBCL was defined as the shortest S1-S1 pacing interval that resulted in 1:1 atrioventricular
218 conduction. AVNERP was defined as the shortest S1-S2 pacing interval that resulted in 1:1
219 atrioventricular conduction. Electrophysiology studies were performed using a Bloom Classic
220 electrophysiology stimulator (Fisher Medical) set to a pacing current 1.5x the minimum pacing
221 threshold, with 1 msec monophasic pulse width. For each parameter, the pacing cycle length
222 (PCL) was decremented to pinpoint the PCL before loss of capture was observed.

223

224 Statistical Analysis

225 Results are reported as mean \pm standard deviation. Data normality was assessed by Shapiro-
226 Wilk testing (Graphpad Prism). Statistical analysis was performed using one-way analysis of
227 variance (ANOVA) for microelectrode array recordings or two-way analysis of variance with
228 repeated measures (RM-ANOVA) to compare baseline vs treatment in whole heart experiments.
229 Significance was defined by an adjusted p-value ($q < 0.1$) after multiple comparisons testing with
230 a false discovery rate of 0.1; significance is denoted in the figures with an asterisk (*).

231 **RESULTS**

232 **BPA exerts a greater inhibitory effect on ion channels, compared with BPS or BPF**

233 Whole-cell voltage clamp recordings were performed on cells transfected with one of four
234 cardiac ion channels, as highlighted by CiPA (Colatsky et al. 2016; Sager et al. 2014). Currents
235 were evoked and recorded before and after exposure to BPA, BPS, or BPF, and a half-maximal
236 inhibitory concentration (IC_{50}) was computed by testing the respective affinities to each ion
237 channel. Collectively, BPA had the highest affinity for each ion channel tested, compared to
238 both BPF and BPS, and current suppression was concentration dependent (**Figure 2,3**). Peak
239 sodium current (I_{Na-P}) was suppressed with an IC_{50} of 55.3 μ M BPA, 232 μ M BPF, and 1090 μ M
240 for BPS; late sodium current (I_{Na-L}) was suppressed at lower doses, with a computed IC_{50} of 23.6
241 μ M BPA, 100 μ M BPF, and 369 μ M BPS (**Figure 2A,B**). In ventricular tissue, I_{Na-P} is responsible
242 for action potential upstroke (phase 0) and I_{Na-L} is involved in the plateau phase (phase 2).
243 Accordingly, inhibition of I_{Na-P} is likely to slow depolarization and electrical conduction, while
244 inhibition of I_{Na-L} can shorten the action potential duration. L-type calcium channel current (I_{CaL})
245 was also the most sensitive to BPA exposure, with an IC_{50} of 30.8 μ M, compared to 76 μ M BPF
246 and 333 μ M BPS (**Figure 3A**). In ventricular myocytes, calcium current (I_{CaL}) plays a prominent
247 role in the plateau phase, and also contributes to the action potential upstroke in nodal cells.
248 Inhibition of I_{CaL} can slow sinus rate, delay atrioventricular conduction, and shorten the
249 ventricular myocyte action potential. Finally, the rapid delayed rectifier potassium current (I_{Kr})
250 was suppressed at higher bisphenol concentrations, with a measured IC_{50} of 127 μ M BPA, 209
251 μ M BPF, and 633 μ M BPS (**Figure 3B**). Bisphenol exposure could suppress I_{Kr} and prolong
252 cardiac repolarization (phase 3) at high concentrations.

253

254 **BPA and BPF exposure alters the extracellular field potential of human cardiomyocytes**

255 To validate the effects of bisphenol chemicals on cardiac electrophysiology, we employed
256 hiPSC-CM that express key cardiac ion channels (Edwards and Louch 2017). hiPSC-CM were
257 cultured atop microelectrodes and extracellular field potentials were recorded (**Figure 4A, D, G**),
258 with FPD measurements analogous to an *in vitro* QT interval that correlates with the action
259 potential duration (Asakura et al.; Clements 2016). Acute BPA exposure resulted in a slight non-
260 monotonic dose response (**Figure 4B**), wherein no effect on FPDc was observed at the lowest
261 BPA dose tested (0.01 μ M) and a 7.5% increase in FPDc was observed at 100 nM BPA
262 ($q < 0.005$). Notably, low dose effects have previously been reported for BPA and other
263 endocrine-disrupting chemicals that can present with a non-monotonic dose response
264 (Birnbaum 2012; Vandenberg 2014). At higher BPA doses, FPDc shortened significantly

265 compared to the vehicle (13.8% at 30 μ M, 37.3% at 100 μ M, $q < 0.0001$). Low dose effects were
266 not observed for either BPF or BPS (**Figure 4E, H**). However, BPF exposure resulted in FPDc
267 shortening at higher concentrations (3.7% at 10 μ M ($q < 0.05$), 12.5% at 30 μ M ($q < 0.0001$),
268 32.4% at 100 μ M ($q < 0.0001$)). Treatment with BPS did not alter FPDc at any of the tested
269 concentrations. FPDc restitution curves were generated by increasing the pacing frequency (1-2
270 Hz). A frequency-dependent effect was not observed for BPA in hiPSC-CM, although BPF
271 exhibited a slight reverse-use dependency with FPDc shortening more prominent at slower
272 frequencies (**Figure 4C, F**).

273

274 **BPA and BPF exposure slows heart rate**

275 To aid in the translation of our *in vitro* findings, we quantified the acute effects of BPA, BPF, and
276 BPS on cardiac electrophysiology using an *ex vivo* intact heart preparation. Heart preparations
277 exhibited normal sinus rhythm when perfused with control KH media (327.7 ± 36.8 BPM) and
278 KH media supplemented with vehicle (327.6 ± 40.3 BPM; **Figure 1C**). BPA exposure resulted in
279 a measurable decline in heart rate, which may be partly attributed to calcium channel current
280 inhibition. Sinus rate slowed by 16.6% ($q < 0.01$) and 85.4% ($q < 0.0001$) after exposure to 10 μ M
281 and 100 μ M BPA, respectively (relative to baseline recording; **Figure 5A,B**). This depressive
282 effect culminated in cessation of ventricular electrical activity in 62% of heart preparations
283 treated with 100 μ M BPA (**Figure 5D**). Heart rate slowing was immediate, yet reversible, as
284 sinus rhythm recovered quickly after removal of BPA and replacement with control media
285 perfusion. A non-monotonic BPA dose response relationship was not observed. Heart rate also
286 slowed by 12.5% ($q < 0.001$) after exposure to 100 μ M BPF, the only dose to significantly affect
287 automaticity (**Figure 5E**). Conversely, no significant change in sinus rhythm or rate were
288 observed after exposure to BPS (**Figure 5G**).

289

290 **BPA and BPF exposure slows atrioventricular conduction**

291 Heart preparations exhibited stable atrial and atrioventricular conduction with control media
292 perfusion (15.3 ± 2.8 msec P duration, 33.6 ± 1.4 msec PR interval), and during perfusion with
293 media supplemented with vehicle (16.3 ± 4.0 msec P duration, 35.3 ± 3.1 msec PR interval).
294 Concurrent with heart rate slowing due to BPA exposure, we also observed significant
295 lengthening of both the P duration and PR interval. A prolonged P duration was only observed
296 at the highest BPA dose (39.8 ± 16.6 msec at 100 μ M BPA, **Figure 6B**), whereas the PR
297 interval progressively lengthened with higher BPA concentrations (**Figure 6A, D**). BPA
298 exposure resulted in variable degrees of atrioventricular (AV) block, ranging from 1st degree to

299 intermittent 3rd degree AV block (**Figure 6D**). Notably, the acute effect of BPA on AV conduction
300 was reversible with a rapid recovery of the PR interval time after washout (**Figure 6E**). Atrial
301 pacing was implemented, and AV conduction slowing persisted at multiple PCL (**Figure 6F**).
302 BPF exposure also lengthened the PR interval, albeit the effect was much less pronounced
303 (+19.6% 100 μ M BPF). There was no observable change in AV conduction following BPS
304 exposure (**Figure 6I**).

305

306 **BPA and BPF exposure increases atrioventricular nodal refractoriness**

307 To further investigate slowed AV conduction in the presence of bisphenols, incremental atrial
308 pacing was implemented to pinpoint the Wenckebach phenomenon. WBCL was comparable
309 between control media perfusion (87 ± 6.2 msec) and during perfusion with vehicle (90 ± 6.5
310 msec). But, proved to be a highly sensitive parameter for bisphenol-induced slowing of AV
311 conduction (**Figure 7A,B**). BPA exposure altered WBCL in a dose-dependent manner beginning
312 at a low nanomolar concentration (+7.6% 0.01 μ M BPA ($q < 0.1$); +68% 100 μ M BPA
313 ($q < 0.0001$)), suggesting a lengthening of the relative refractory period. Pinpointing an accurate
314 WBCL after 100 μ M BPA exposure was confounded by loss of capture at the slowest cycle
315 length tested (150 msec; **Figure 7C**). BPF exposure had a moderate effect on WBCL, but only
316 at the highest concentration tested (22.5% 100 μ M BPF ($q < 0.0001$)). BPS exposure did not alter
317 WBCL, which was in agreement with PR interval measurements during sinus rhythm (**Figure**
318 **7G**). Extrastimulus pacing was also performed to measure the effective refractory period of the
319 atrioventricular node. Similar to WBCL measurements, BPA exposure increased AV node
320 refractoriness in a dose-dependent manner (**Figure 8A,B**), beginning with modest changes at a
321 low nanomolar concentration (+9.2% 0.001 μ M BPA ($q < 0.05$)) and increasing thereafter
322 (+95.7% 100 μ M BPA ($q < 0.0001$)). BPF exposure had a moderate effect on AVNERP, but only
323 at the highest concentration tested (20.7% 100 μ M BPF ($q < 0.0001$)). BPS exposure did not alter
324 AVNERP (**Figure 8G**).

325

326 **DISCUSSION**

327 This is the first study to compare the direct effects of BPA, BPS, and BPF on cardiac
328 electrophysiology using both *in vitro* and *ex vivo* cardiac preparations. In the described study,
329 we demonstrate that BPA is the most potent inhibitor of sodium, calcium and potassium channel
330 currents – as compared to the chemical alternatives, BPS and BPF. Using a range of
331 concentrations that encompass environmental, clinical, and supraphysiological exposures, we
332 found that BPA exerted the greatest effect on automaticity and atrioventricular conduction.

333 Electrical disturbances were largely focused on nodal and atrioventricular conduction, with
334 negligible effects on cardiac repolarization or arrhythmia susceptibility. Results of this study
335 indicate that BPS is significantly less disruptive to cardiac electrophysiology and may serve as a
336 safer chemical alternative for plastic medical products. It is important to note that in the context
337 of industrial or clinical environments, individuals can present with urinary BPA concentrations
338 that are exceedingly high – reaching 4-8 μM (Calafat et al. 2009; He et al. 2009; Wang et al.
339 2012). Notably, this study focused on acute bisphenol exposure and the direct impact on
340 cardiac electrophysiology endpoints; as such, we did not investigate intracellular signaling or
341 possible genomic effects of bisphenol chemicals. Additional mechanistic studies are required to
342 fully elucidate the safety profile of bisphenol chemicals on cardiac electrical and mechanical
343 function, and report on the chronic effects of bisphenol exposure.

344

345 Bisphenol chemicals and calcium ion homeostasis

346 Of the bisphenol chemicals tested in this study, BPA was the most potent inhibitor of L-type
347 calcium channels with an $\text{IC}_{50} = 30.8 \mu\text{M}$. This finding is in agreement with the literature, which
348 reported an immediate, inhibitory effect of BPA on T-type calcium channels in HEK cells ($\text{IC}_{50} =$
349 $6\text{-}33 \mu\text{M}$, depending on channel subtype; (Michaela et al. 2014)). Similarly, Deutschmann, et al.
350 reported that BPA rapidly and reversibly inhibited calcium current through L-, N-, P/Q-, R-, and
351 T-type calcium channels in rat endocrine cells, dorsal root ganglion, cardiomyocytes, and
352 transfected HEK cells ($\text{IC}_{50} = 26\text{-}35 \mu\text{M}$; (Deutschmann et al. 2013)). Studies suggest that the
353 inhibitory effect of bisphenol chemicals on calcium channel current are influenced by the
354 chemical structure and bridge between the two phenol rings, with reduced inhibitory effects
355 anticipated for BPS and BPF (Deutschmann et al. 2013). In cardiac tissue, calcium channels
356 play an important role in nodal cell depolarization, atrioventricular conduction, the plateau phase
357 of the cardiac action potential, and contractility. Indeed, recent studies have shown that BPA
358 can alter cardiac electrophysiology, likely through a calcium-dependent mechanism. Sinus
359 bradycardia and delayed electrical conduction have been reported after BPA exposure, using *in*
360 *vivo* and *ex vivo* models (Belcher et al. 2015; Patel et al. 2015; Posnack et al. 2014; Valokola et
361 al. 2019). Patel et al. observed conduction slowing in BPA-exposed animals subjected to
362 catecholamine stress, although this effect was limited to females (Patel et al. 2015). BPA-
363 induced heart rate slowing was also reported in *in vivo* studies conducted by Belcher, et al.,
364 although the authors noted that this effect may be attributed to autonomic dysregulation
365 (Belcher et al. 2015). In addition to electrophysiology disturbances, BPA-exposure has been
366 shown to alter intracellular calcium handling, which can increase calcium leak from the

367 sarcoplasmic reticulum (Yan et al. 2011), increase the incidence of calcium-mediated
368 arrhythmias, and precipitate calcium amplitude alternans (Ramadan et al. 2018). Studies
369 suggest that intracellular calcium handling may be influenced by posttranslational modifications
370 of key calcium proteins, via an estrogen-mediated mechanism (Liang et al. 2014).

371

372 Bisphenol chemicals and sodium channel current

373 Similar to calcium channel inhibition, we found that BPA was the most potent inhibitor of fast
374 (I_{Na-P}) and late (I_{Na-L}) sodium channel ($IC_{50} = 55.3$ and $23.6 \mu M$, respectively). This finding is in
375 agreement with previously published studies, which reported that BPA blocks fast-voltage gated
376 sodium channels in transfected HEK cells ($IC_{50} = 25 \mu M$; (O'Reilly et al. 2012)) and isolated
377 dorsal root ganglion neurons ($IC_{50} = 40 \mu M$; (Wang et al. 2011)). These effects were rapid,
378 reversible, and dose-dependent (Wang et al. 2011). Moreover, in isolated ganglion neurons, the
379 described effects were attenuated with protein kinase A (PKA) or protein kinase C (PKC)
380 inhibitors, suggesting an underlying protein-kinase dependent pathway. In cardiac tissue, the
381 fast voltage-gated sodium channel (I_{Na-P} ; TTX-sensitive) is responsible for the action potential
382 upstroke and blockade is likely to reduce the rate of depolarization and slow conduction velocity.
383 Late-sodium channel current (TTX-insensitive) is active during the action potential plateau
384 phase, and blockade is expected to shorten repolarization time, which in turn, reduces calcium
385 channel current (Horváth et al. 2020). This highlights the importance of performing
386 electrophysiology studies using cardiac models (e.g., human cardiomyocytes, isolated whole
387 heart, in vivo studies) in conjunction with single channel studies, given the dynamic nature of
388 cardiac electrophysiology.

389

390 Bisphenol chemicals and estrogen-receptor signaling

391 Since BPA is classified as a xenoestrogen, alterations in cardiac function may also be attributed
392 to its interaction with estrogen receptors. In the presented study, we utilized female cardiac
393 preparations since previous reports have indicated that BPA-induced effects on calcium
394 handling and electrical instabilities can be heightened in female animals, exacerbated in the
395 presence of estradiol, and attenuated in ER β knockout animals (Belcher et al. 2011; Yan et al.
396 2011). Further, studies have shown that 17 β -estradiol alone can rapidly and reversibly inhibit
397 sodium and calcium channels, in a concentration dependent manner (DY et al. 2002; Wang et
398 al. 2013). Accordingly, the effects of BPA on cardiac electrophysiology may be mediated by
399 direct interaction with ion channels at the cell membrane and/or intracellular signaling pathways
400 precipitated by estrogen receptor binding. Of interest, BPS and BPF have also been shown to

401 display estrogenic activity that is comparable to BPA (Kojima et al. 2019; Moreman et al. 2017).
402 Although in the presented study, we identified clear differences in the potency of BPA, BPS, and
403 BPF as it relates to ion channel inhibition and cardiac electrophysiology parameters.

404

405 Cardiac safety profile of bisphenol A analogues

406 Biomonitoring studies have recently reported an uptick in BPS and BPF exposure in the general
407 population, as manufacturers begin to phase out and replace BPA in some consumer and
408 medical products. As an example, data from the 2013-2014 National Health and Nutrition
409 Examination Survey (NHANES) detected BPA, BPS, and BPF in 96%, 90%, and 67% of urinary
410 samples from the general population (Lehmle et al. 2018). Yet, very little is known about the
411 effects of these substitute chemicals on cardiovascular health, and whether they offer a superior
412 safety profile. Using a zebrafish model, Chen et al. reported that BPS exposure results in
413 transcriptional changes that can increase inflammation, alter cardiac morphology, and *decrease*
414 heart rate (Qiu et al. 2020). In a rodent cardiac model, BPS-treatment alone was shown to
415 *increase* heart rate, while the addition of catecholamine stress increased the propensity for
416 premature ventricular contractions and calcium-mediated triggered activity (Gao et al. 2015).
417 The authors noted that the observed effect on cardiac electrophysiology was sex-specific and
418 mediated via estrogen receptor- β signaling, which alters the phosphorylation status of key
419 calcium handling proteins. Notably, the same group has reported nearly identical effects with
420 BPA-treatment, which suggest that the two chemicals may act via a common mechanism (Yan
421 et al. 2011). In a separate study by Ferguson, et al., BPS or BPA-treatment rapidly reduced
422 mechanical function in heart preparations, but slightly different post-translational modifications
423 were observed in myofilament proteins (Ferguson et al. 2019). Investigations into the cardiac
424 effects of BPF are even more limited, with a single report noting a decrease in the heart rate of
425 zebrafish following BPF-exposure (Mu et al. 2019). The current study was focused on cardiac
426 electrophysiology outcomes, therefore, additional work is needed to assess the impact of BPA,
427 BPF, and BPS on myocardial contractility.

428

429 To the best of our knowledge, our study is the first to compare the acute effects of BPA, BPS,
430 and BPF exposure on cardiac electrophysiology. We aimed to identify the IC_{50} concentrations
431 for BPA, BPS, and BPF on key cardiac ion channels highlighted by the CiPA initiative – and
432 validate the effect of those concentrations on human cardiomyocyte and intact heart
433 preparations. Collectively, we observed that BPA exposure has a more potent effect on cardiac
434 electrophysiology, as compared to the chemical substitutes BPF and BPS. Our results suggest

435 that BPS may be a safer chemical alternative, particularly for medical devices that are used to
436 treat vulnerable patient populations that are at increased risk for bisphenol chemical exposure.
437 Nevertheless, a few limitations to our study should be considered. Although we included a
438 number of models in our study, further in-depth mechanistic work is necessary to fully elucidate
439 the safety profile of bisphenol chemicals – including the impact on intracellular targets, genomic
440 and proteomic expression profiles (sub-acute or chronic studies), and autonomic regulation (in
441 vivo studies). There are also notable differences in cardiac electrophysiology between rodents
442 and humans (e.g., ion channel expression, sinus rate, action potential morphology) which
443 should be noted when considering the translation of experimental studies to humans.

444

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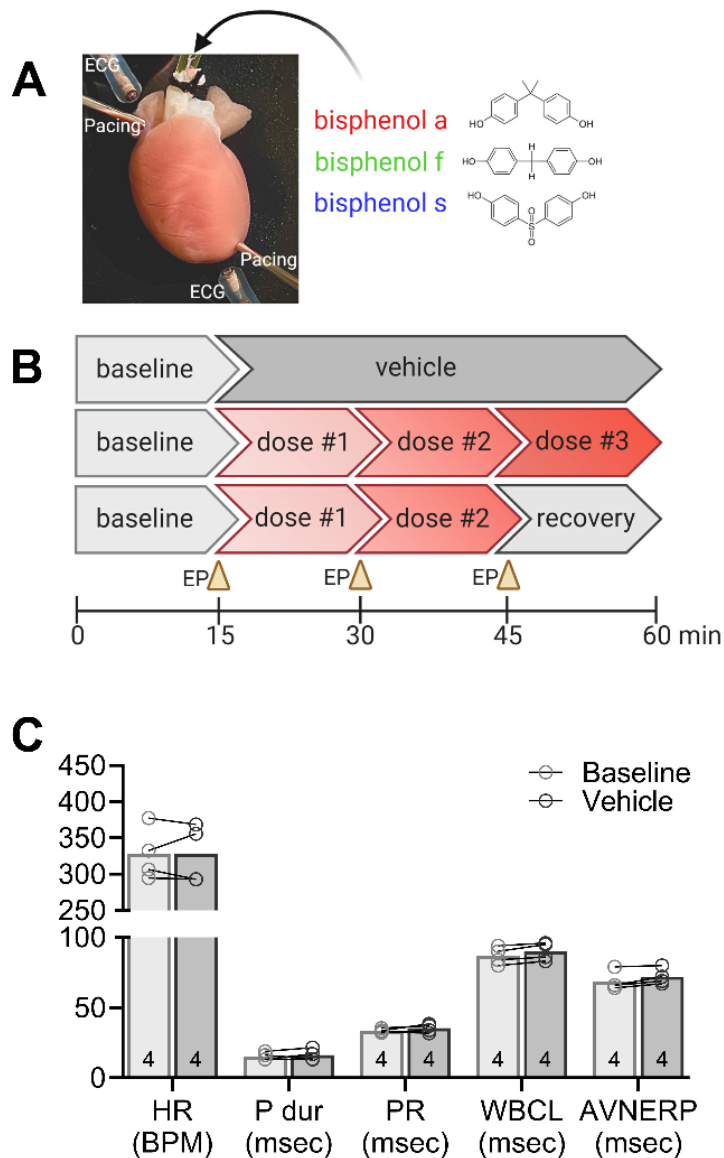
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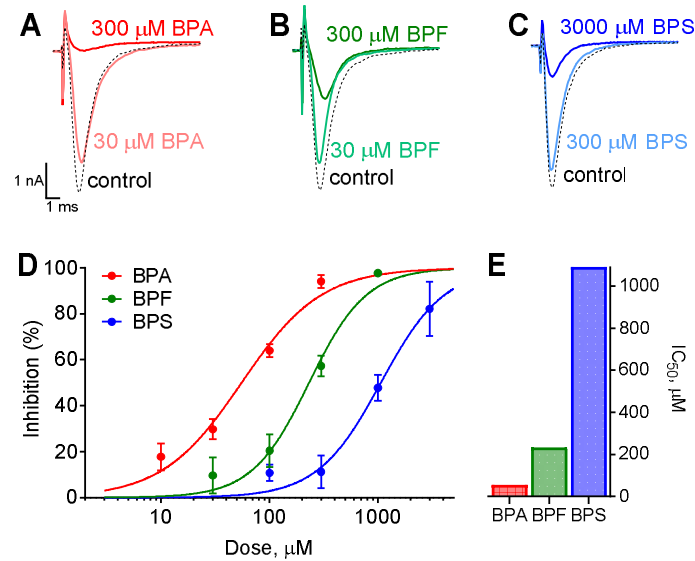
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649 **Figure Legends**

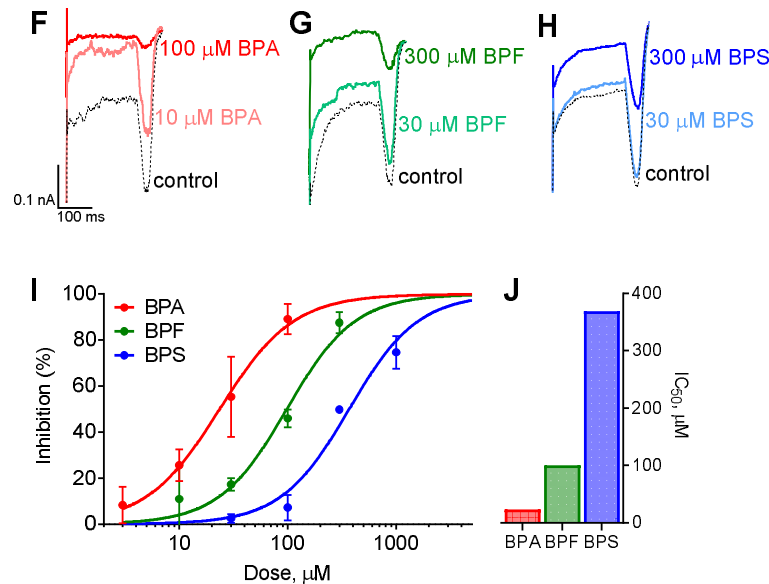


650 **Figure 1. Experimental design and vehicle control parameters.** (A) Langendorff-perfused rat
 651 heart shown with pacing electrodes on the right atria and apex, and monopolar electrodes
 652 placed to record electrocardiograms. (B) Schematic timeline depicts perfusion protocols used in
 653 the study, including (top) vehicle control exposure, (middle) bisphenol chemical dose response,
 654 (bottom) bisphenol chemical dose response and subsequent recovery. (C) Cardiac
 655 electrophysiology parameters are consistent over time, and similar between baseline and
 656 vehicle (0.01% DMSO) exposure. Values reported as mean \pm SD. Statistical significance
 657 determined by RM-ANOVA with multiple comparisons testing (0.1 FDR). Number of replicates
 658 indicated in each bar graph (n=4). ECG = location of electrocardiogram electrode, EP =
 659 electrophysiology protocol, HR = heart rate, BPM = beats per minute, P dur = P wave duration,
 660 PR = PR interval, WBCL = Wenckebach cycle length, AVNERP = atrioventricular node effective
 661 refractory period, msec = milliseconds

Nav1.5 (I_{Na-P}) current

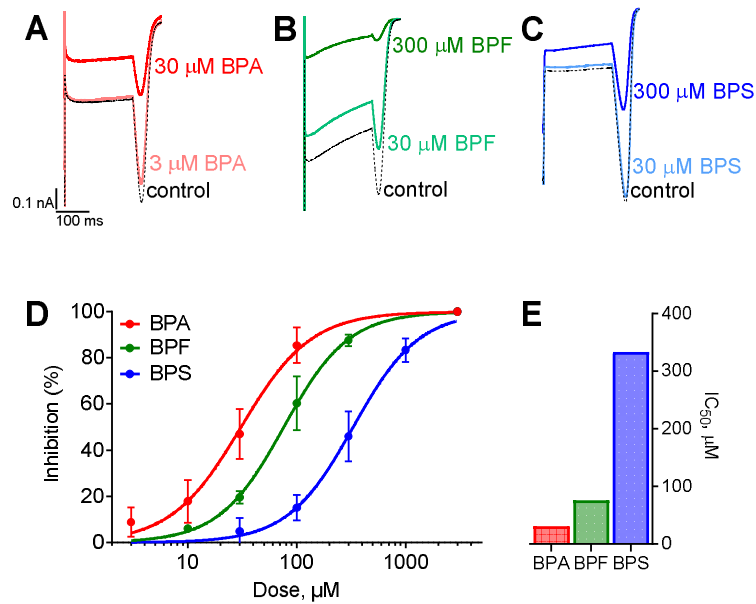


Nav1.5 (I_{Na-L}) current

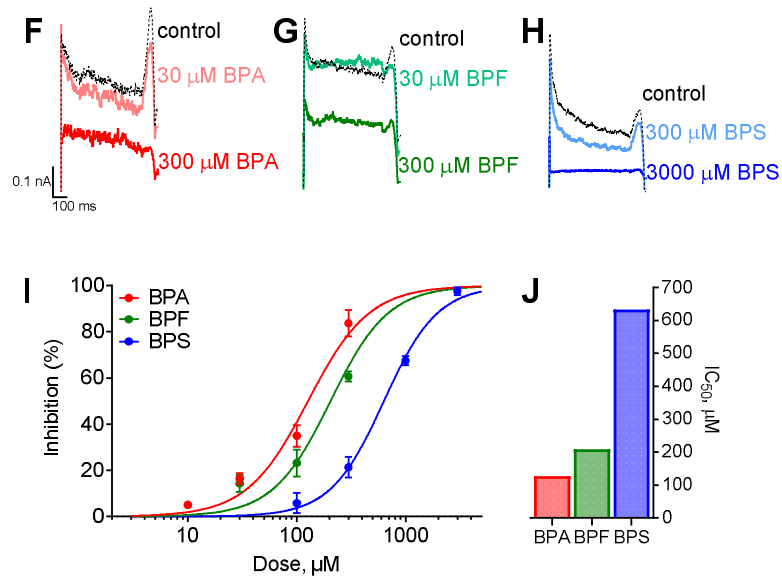


662 **Figure 2. Bisphenol inhibition of sodium currents.** Whole-cell voltage clamp recordings of
663 fast/peak sodium current (I_{Na-P}) following exposure to (A) BPA, (B) BPF, or (C) BPS. (D) Dose-
664 dose-dependent inhibition of I_{Na-P} (mean \pm SD). (E) Calculated IC_{50} values are shown. Whole-cell
665 voltage clamp recordings of late sodium current (I_{Na-L}) following exposure to (F) BPA, (G) BPF,
666 or (H) BPS. (I) Dose-dependent inhibition of I_{Na-L} (mean \pm SD). (J) Calculated IC_{50} values are
667 shown.
668

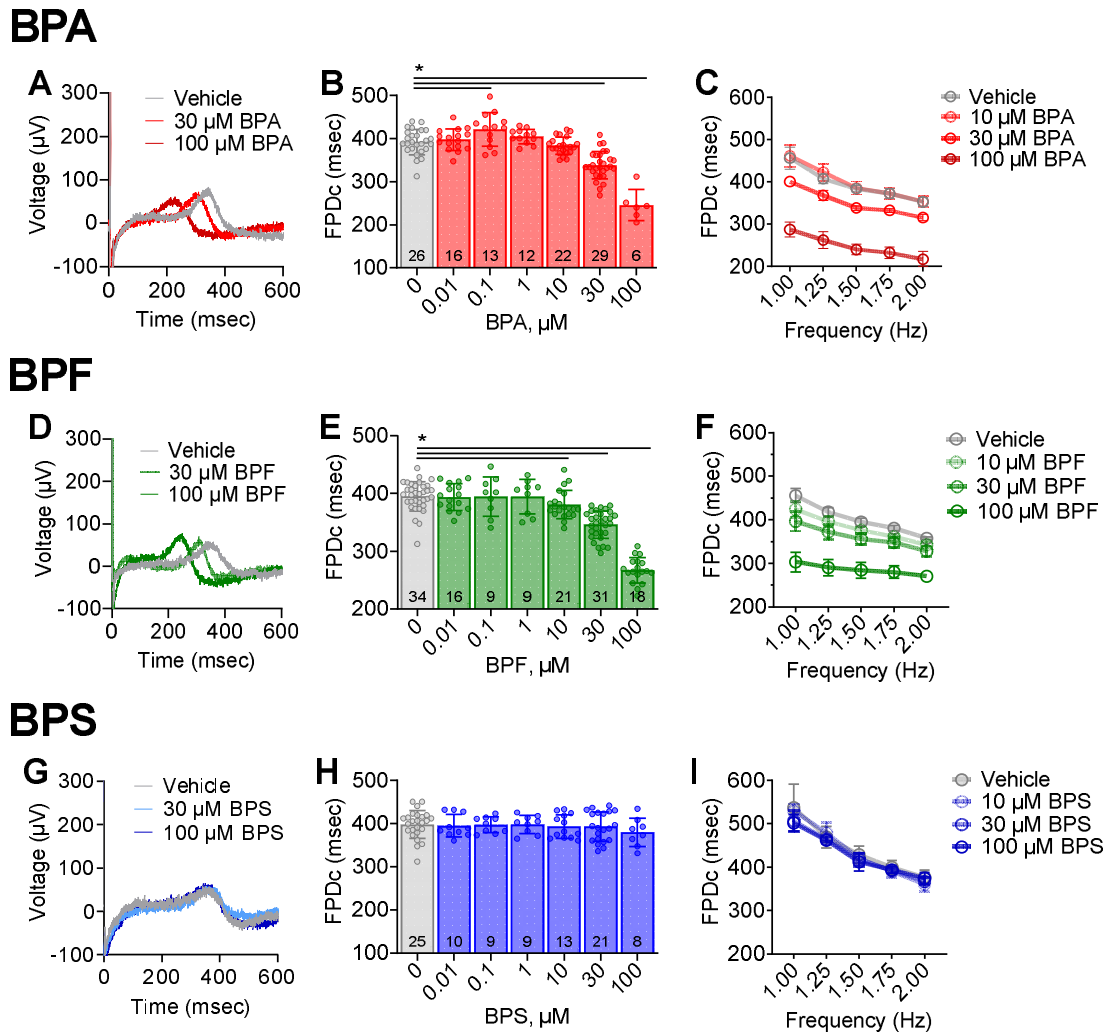
CaV1.2 (I_{CaL}) current



hERG (I_{Kr}) current



669 **Figure 3. Bisphenol inhibition of calcium and potassium currents.** Whole-cell voltage
670 clamp recordings of L-type calcium current (I_{CaL}) following exposure to **(A)** BPA, **(B)** BPF, or **(C)**
671 BPS. **(D)** Dose-dependent inhibition of I_{CaL} (mean \pm SD). **(E)** Calculated IC_{50} values are shown.
672 Whole-cell voltage clamp recordings of hERG current (I_{Kr}) following exposure to **(F)** BPA, **(G)**
673 BPF, or **(H)** BPS. **(I)** Dose-dependent inhibition of I_{Kr} (mean \pm SD). **(J)** Calculated IC_{50} values
674 are shown.

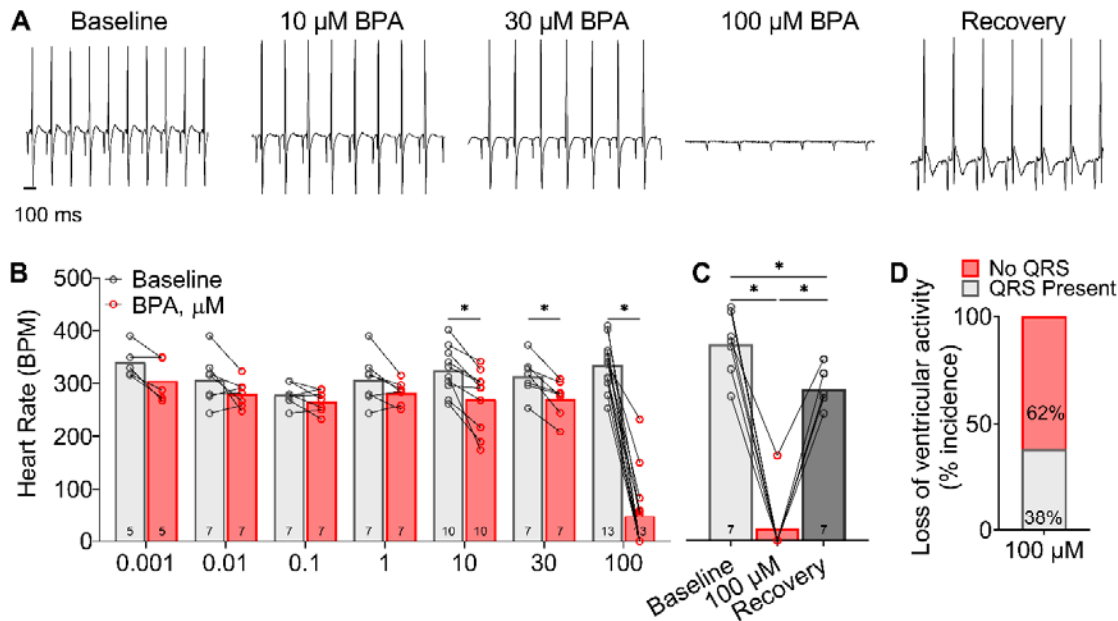


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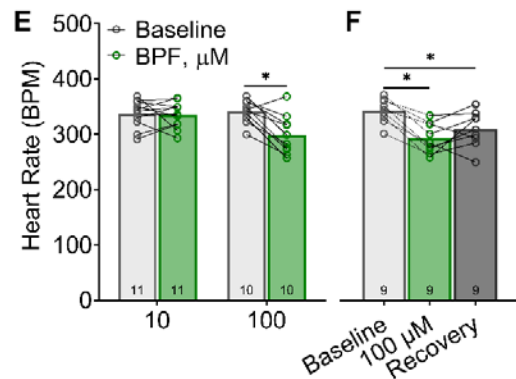
676 **Figure 4. Cardiomyocyte field potential duration shortens with BPA or BPF exposure, but**
 677 **not BPS. (A)** Representative traces of extracellular field potentials recorded from hiPSC-CM
 678 following acute exposure to vehicle, 30 μ M, or 100 μ M BPA. **(B)** Field potential duration
 679 (corrected using Frederica formula: 'FPDc') shortens with increasing BPA exposure; single
 680 pacing frequency (1.5 Hz). **(C)** FPDc restitution curve at multiple pacing frequencies (1-2 Hz).
 681 **(D)** Local field potential traces following exposure to vehicle, 30 μ M, or 100 μ M BPF. **(E)** FPDc
 682 shortens with increasing BPF exposure (1.5 Hz). **(F)** FPDc restitution curve (1-2 Hz). **(G)** Local
 683 field potential traces following exposure 30-100 μ M BPS. **(H)** FPDc remains constant with
 684 increasing BPS exposure (1.5 Hz). **(I)** FPDc restitution curve (1-2 Hz). Values reported as mean
 685 \pm SD. * $q < 0.05$ as determined by ANOVA with multiple comparisons testing (0.1 FDR). Number
 686 of replicates indicated in each bar graph.

687

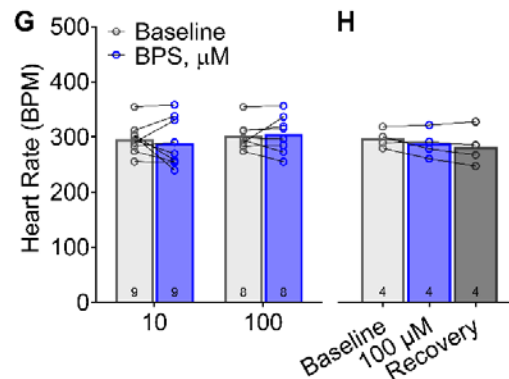
BPA heart rate



BPF heart rate

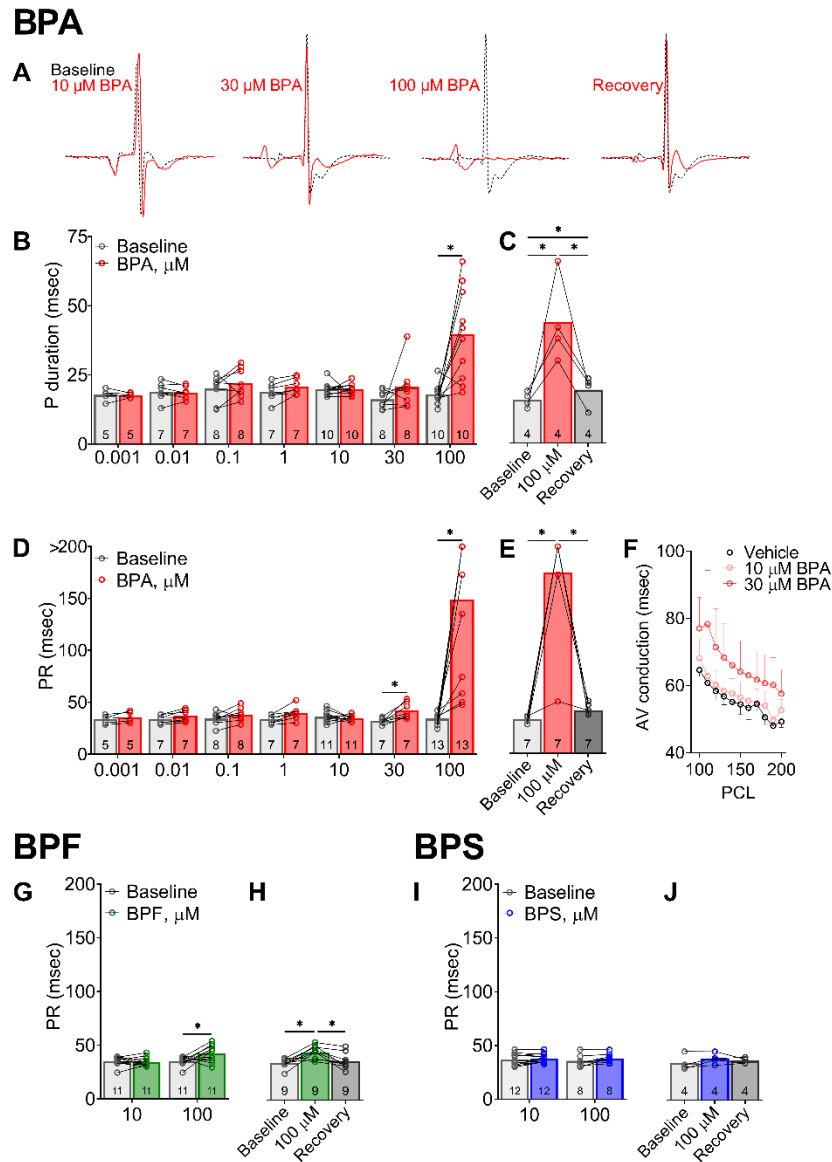


BPS heart rate



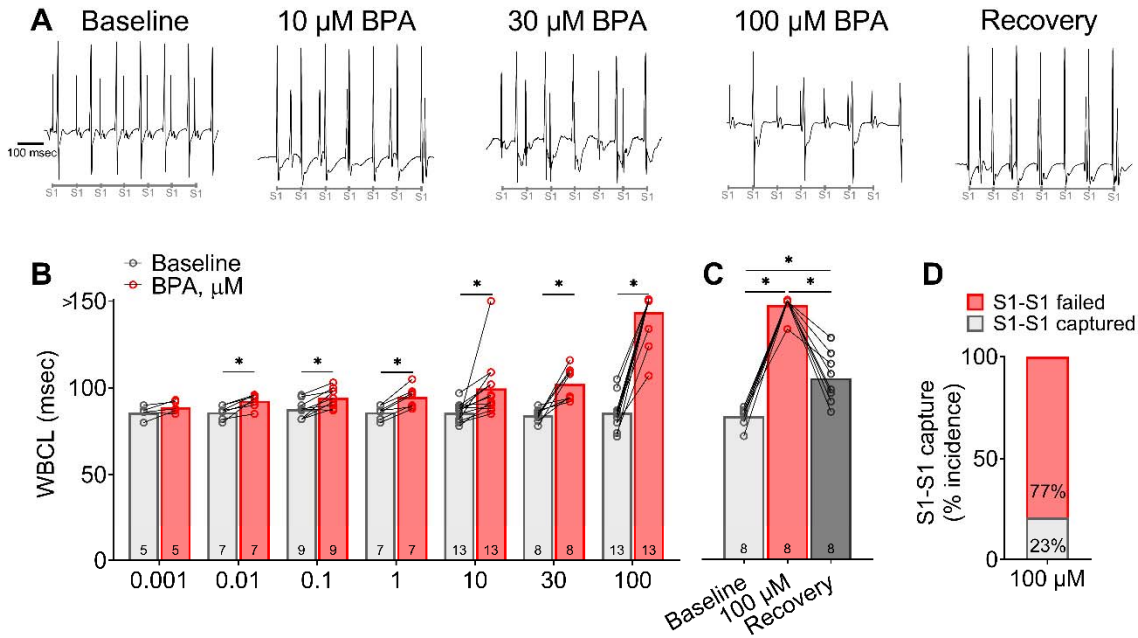
688

689 **Figure 5. Heart rate slows in the presence of BPA or BPF exposure, but not BPS. (A)**
 690 Representative ECG recordings from Langendorff-perfused hearts at baseline, acute (15 min)
 691 exposure to BPA, or recovery (100 μM BPA exposure, followed by 15 min washout). **(B)**
 692 BPA exposure results in sinus rate slowing, beginning at 10 μM BPA. **(C)** Heart rate slowing after 100
 693 μM BPA exposure largely recovers after washout (15 min). **(D)** Heart rate measurements at high
 694 BPA doses were confounded by intermittent 3rd degree heart block, with loss of ventricular
 695 electrical activity. **(E)** Heart rate slowing following BPF exposure occurred only at highest
 696 concentration tested (100 μM BPF). **(F)** Heart rate slowing after 100 μM BPF recovered slightly
 697 after washout. **(G,H)** BPS exposure had no discernable effect on heart rate. Values reported as
 698 mean \pm SD. * $q < 0.05$ as determined by RM-ANOVA with multiple comparisons testing (0.1
 699 FDR). Number of replicates indicated in each bar graph.

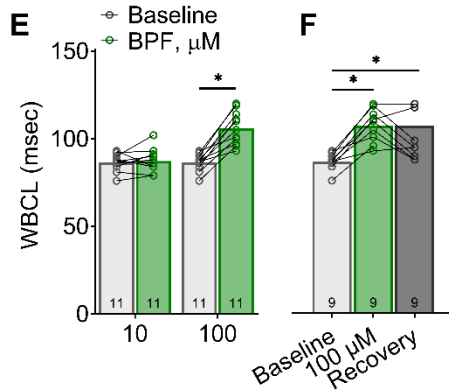


700 **Figure 6. Atrial and atrioventricular conduction slows with BPA and BPF exposure, but**
 701 **not BPS. (A)** Representative ECG waveform from Langendorff-perfused hearts at baseline,
 702 acute BPA exposure (15 min), or recovery (100 μ M BPA exposure, followed by 15 min
 703 washout). Each waveform pair recorded from the same animal, before and after exposure. **(B)**
 704 P duration indicates longer atrial depolarization time at highest BPA dose (100 μ M). **(C)**
 705 Slowed atrial conduction after 100 μ M BPA exposure recovers after washout. **(D)** Progressive
 706 lengthening of PR duration indicates slowed AV conduction following 30-100 μ M BPA exposure,
 707 often resulting in intermittent 3rd degree heart block (denoted by data point >200 msec). **(E)**
 708 AV conduction slows after 100 μ M BPA exposure and recovers after washout. **(F)** AV conduction
 709 slowing persists with external pacing to correct for heart rate. **(G)** Atrioventricular conduction
 710 slowing occurs only at highest BPF concentration (100 μ M) and **(H)** recovers after washout. **(I,J)**
 711 BPS exposure had no discernable effect on atrioventricular conduction time. Values reported as
 712 mean \pm SD. * $q < 0.05$ as determined by RM-ANOVA with multiple comparisons testing (0.1
 713 FDR). Number of replicates indicated in each bar graph. PCL= pacing cycle length

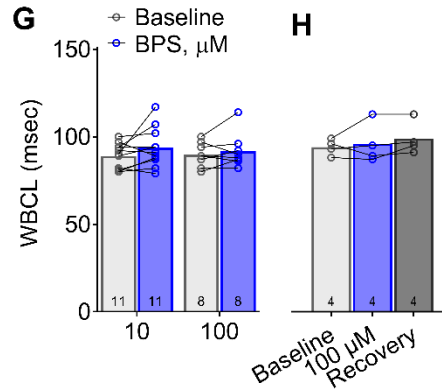
BPA WBCL



BPF WBCL

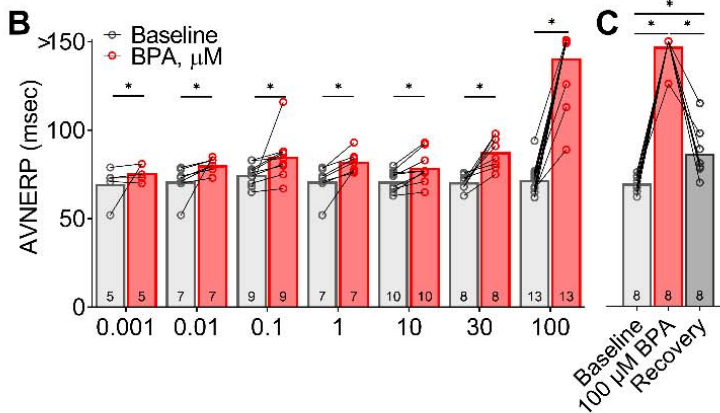
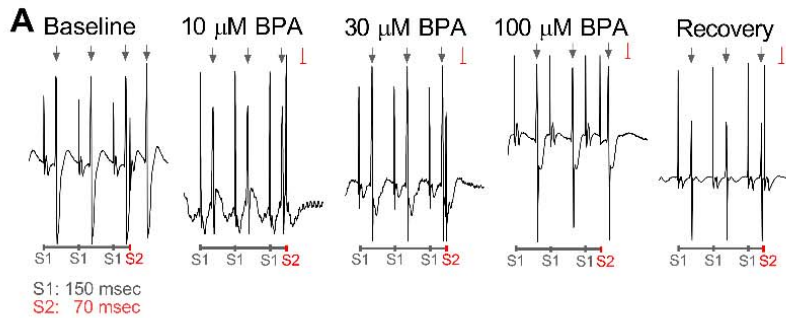


BPS WBCL

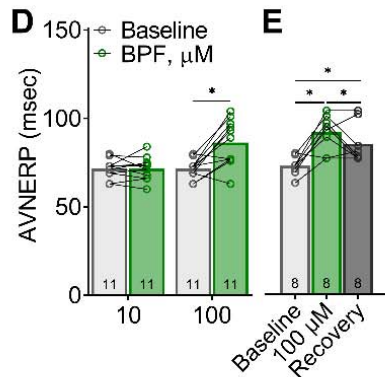


714 **Figure 7. Atrial pacing highlights atrioventricular slowing after BPA or BPF, but not BPS**
 715 **exposure. (A)** Representative ECG recordings during atrial pacing show failure to capture in
 716 BPA-treated hearts, indicating slowed atrioventricular conduction. Timing of S1-S1 pulses (90
 717 msec) are indicated below. **(B)** Longer Wenckebach cycle length (WBCL) following exposure to
 718 BPA concentrations (0.01–100 μM), as compared with baseline. Note: Complete Heart block
 719 denoted by measurement >150 msec (longest S1 pacing interval tested). **(C)** Longer WBCL
 720 after 100 μM BPA exposure largely recovers after washout. **(D)** WBCL measurements at high
 721 BPA doses were confounded by complete heart block. **(E)** Only 100 μM BPF exposure results in
 722 longer WBCL. **(F)** Moderate recovery in atrioventricular conduction after BPF washout. **(G,H)** No
 723 change in WBCL was observed after exposure to BPS. Values reported as mean \pm SD. * $q < 0.05$
 724 as determined by RM-ANOVA with multiple comparisons testing (0.1 FDR). Number of
 725 replicates indicated in each bar graph.

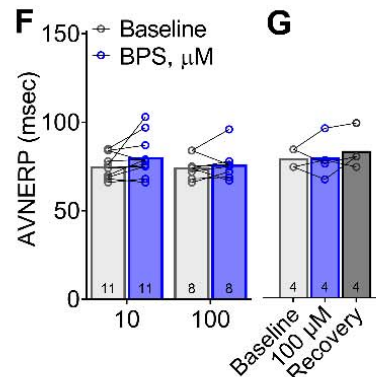
BPA AVNERP



BPF AVNERP



BPS AVNERP



726 **Figure 8. Increased atrioventricular nodal refractoriness after exposure to BPA and BPF,**
 727 **but not BPS. (A)** Representative ECG recordings during atrial pacing show capture (\downarrow) and
 728 failure to capture (\uparrow) in response to S1-S2 pacing (150, 70 msec). **(B)** Longer atrioventricular
 729 nodal effective refractory period (AVNERP) following exposure to BPA concentrations (1–100
 730 μ M), as compared with baseline. Note: Complete heart block denoted by measurement >150
 731 msec (S1 pacing interval). **(C)** Longer AVNERP after 100 μ M BPA exposure recovers after
 732 washout. **(D)** BPF exposure results in longer AVNERP, but only at highest dose tested. **(E)**
 733 Moderate recovery of AVNERP after BPF washout. **(F,G)** No change in AVNERP was observed
 734 after exposure to BPS. Values reported as mean \pm SD. * $q < 0.05$ as determined by RM-ANOVA
 735 with multiple comparisons testing (0.1 FDR). Number of replicates indicated in each bar graph.