

# Altered effective connectivity in sensorimotor cortices: a novel signature of severity and clinical course in depression

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This manuscript was compiled on June 30, 2021

1 **Functional neuroimaging research on depression has traditionally**  
2 **targeted neural networks associated with the psychological aspects**  
3 **of depression. In this study, instead, we focus on alterations of sensorimotor**  
4 **function in depression. We used resting-state functional**  
5 **MRI data and Dynamic Causal Modeling (DCM) to assess the hypothesis**  
6 **that depression is associated with aberrant effective connectivity within and between**  
7 **key regions in the sensorimotor hierarchy. Using hierarchical modeling of between-subject**  
8 **effects in DCM with Parametric Empirical Bayes we first established the architecture of**  
9 **effective connectivity in sensorimotor cortices. We found that in (interoceptive and**  
10 **exteroceptive) sensory cortices across participants, the backward connections are**  
11 **predominantly inhibitory whereas the forward connections are mainly excitatory in**  
12 **nature. In motor cortices these parities were reversed. With increasing depression severity,**  
13 **these patterns are depreciated in exteroceptive and motor cortices and augmented in the**  
14 **interoceptive cortex: an observation that speaks to depressive symptomatology. We**  
15 **established the robustness of these results in a leave-one-out cross validation analysis**  
16 **and by reproducing the main results in a follow-up dataset. Interestingly, with (non-**  
17 **pharmacological) treatment, depression associated changes in backward and forward**  
18 **effective connectivity partially reverted to group mean levels. Overall, altered effective**  
19 **connectivity in sensorimotor cortices emerges as a promising and quantifiable**  
20 **candidate marker of depression severity and treatment response.**

depression | embodiment | effective connectivity | spectral DCM | predictive processes

1 **T**he search for the neurological bases of depression has  
2 provided many important insights, yet we are far from a  
3 comprehensive, translatable understanding (1–4). This war-  
4 rants further research and, possibly, new approaches.

5 Neuroimaging research on depression largely focuses on  
6 complex affective and psychological components of depression,  
7 the prefrontal cortex and limbic formation being two of the  
8 most investigated brain regions (5). At the network level,  
9 apart from the fronto-limbic circuitry, default mode network,  
10 cognitive control network, and corticostriatal circuits are some  
11 of the major neurocircuits that are known to be involved in  
12 depression (6–19).

13 However, depression is an embodied phenomenon and is  
14 known to cause alterations in several sensorimotor functions.  
15 Persons suffering from depression, for example, are known to  
16 have reduced visual contrast sensitivity (20), impaired audi-  
17 tory processing of non-speech stimuli (21), and increased pain  
18 tolerance for exteroceptive stimulation (22). In addition to

19 these exteroceptive alterations, depression has been shown to  
20 cause interoceptive changes like decreased pain tolerance for in-  
21 teroceptive stimulation (22) and reduced heartbeat perception  
22 accuracy (23). The psychomotor retardation (reduced speed,  
23 slow speaking rate, delayed motor initiation, body immobility,  
24 loss of facial expression (24)) is a prominent feature of  
25 depression. Indeed, psychomotor retardation has been played  
26 an important role in the descriptive characterization of depres-  
27 sion and melancholia since their nosological inception (24–29).  
28 Darwin (30) described overt psychomotor symptoms in sad  
29 people who “no longer wish for action but remain motionless  
30 and passive, or may occasionally rock themselves to and fro”.  
31 In the following decades, scholars such as Emil Kraepelin de-  
32 veloped the concept further and established its clinical utility  
33 (25, 26). Among later researchers, Carl Wernicke (31), Karl  
34 Kleist (32) and Karl Leonhard (33) contributed to our refined  
35 understanding of psychomotor abnormalities. Lastly, rumina-  
36 tion, an important feature of depression (34), has prominent  
37 sensorimotor components.

38 Although there are a few neuroimaging studies of sensori-  
39 motor changes in depression, our understanding of sensory and  
40 motor function of brain is undergoing a paradigm shift. Spear-  
41 headed by predictive coding and related theoretical frame-

## Significance Statement

Research into neurobiology of depression primarily focuses on its complex psychological aspects. Here, we propose an alternative approach and target sensorimotor alterations - a prominent but often neglected feature of depression. We demonstrated using resting-state fMRI data and computational modelling that top-down and bottom-up information flow in sensory and motor cortices is altered with increasing depression severity in a way that is consistent with depression symptoms. Depression associated changes were found to be consistent across sessions, amenable to treatment and of effect size sufficiently large to predict whether somebody has mild or severe depression. These results pave the way for a new avenue of research into the neural underpinnings of mental health conditions.

D.R., and M.D. conceived the present project. D.B., and M.M. performed experiments, and collected data. D.R., and M.D. performed data analysis. M.D., and K.J.F. supervised the project. D.R., and M.D. wrote the manuscript. D.B., M.M., and K.J.F. edited the manuscript.

The authors declare no competing interest.

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works, there is an emerging consensus among neuroscientists that perception is not a simple ‘bottom-up’ mechanism of progressive abstraction of sensory input (35–37). Bottom-up, top-down and intrinsic neuronal message passing play distinct but crucial roles. This general idea is also applicable to motor function (see active inference (38)). Motivated by these novel insights, we analysed effective connectivity (spectral dynamic causal modelling (39)) in resting state functional MRI data among hierarchical sensorimotor regions in unmedicated depression patients and neurotypical individuals. For exteroceptive perception, effective connectivity among the lateral frontal pole - one of the terminal regions of sensory relays - and primary visual, auditory, and somatosensory cortices was considered. Effective connectivity between anterior and posterior insula was characterised for interoception and between supplementary motor area and primary motor cortex was analysed for motor function (Figure 4). Both group mean effective connectivity and connections showing significant association with Beck Depression Inventory (BDI) scores (40) (after controlling for age and sex) were identified. In a leave-one-out cross-validation (41) - using parametric empirical Bayesian - the effect size was estimated. A subset of participants, who were either treated with cognitive behaviour therapy (42), neurofeedback therapy (43) or not treated were scanned again a few months later and same analysis was implemented, with the addition of treatment effect as a covariate.

## Results

### The primary experiment.

**Accuracy of DCM model estimation.** The accuracy of DCM estimates of effective connectivity for individual participants was excellent. Across participants, the minimum percentage variance-explained by DCM - when fitted to the observed (cross spectra) data - were 73.55%, 68.84%, and 55.00% for left motor, exteroceptive, and interoceptive networks, respectively. For right hemisphere ROIs, these values were 63.2%, 50.79%, and 30.75%. In general, for most participants variance explained was 80% or more.

**Effective connectivity.** Results are displayed in Figure 1 and detailed further in supplementary Figure 1

**Group mean effective connectivity:** The mean effective connectivity among sensorimotor regions is depicted in Figure 1 (a) and (b). Among extensive network of connections in both hemispheres, the most consistent pattern emerged in the forward and backward effective connectivity. In sensory regions (exteroceptive and interoceptive), backward connections were inhibitory, whereas forward connections were excitatory (exception: SSC to FP1 connection). In motor regions, opposite was true (backward: excitatory, forward: inhibitory).

**Changes in effective connectivity with BDI scores:** The connections that showed an association with BDI scores are shown in Figure 1 (c) and (d). As with mean connectivity, the severity associated changes were most consistent in (extrinsic or between region) forward and backward connections across both hemispheres. For exteroceptive and motor cortices, with increasing BDI scores top-down and bottom-up effective connectivity show changes in the opposite direction with respect to group level estimation. For example, in exteroceptive sensory regions (with one exception, see below) bottom-up connections become more negative and top-down connections

become more positive (i.e., disinhibition). In motor regions, top-down connections become more negative and bottom-up connections become more positive. In interoceptive regions top-down inhibitory influences are enhanced.

**Effective connectivity analysis for left auditory regions:** One notable exception to general pattern of changes in exteroceptive sensory regions with BDI scores was found in left auditory regions. Here top-down inhibitory and bottom-up excitatory influences were enhanced with depression. One possible explanation is that this effect reflects enhanced rumination and self-speech in depression (please note that the left auditory cortex is specialized for speech perception). To further probe this hypothesis we implemented spectral DCM analysis among left thalamus, Broca’s area, left A1, and left FP1 regions. We found that left A1 was driven mainly by Broca’s area rather than the left Thalamus (see second sub-figure below). We will return to this observation in discussion.

### Cross Validation

**Table 1. Leave-one-out cross validation: results from the primary study**

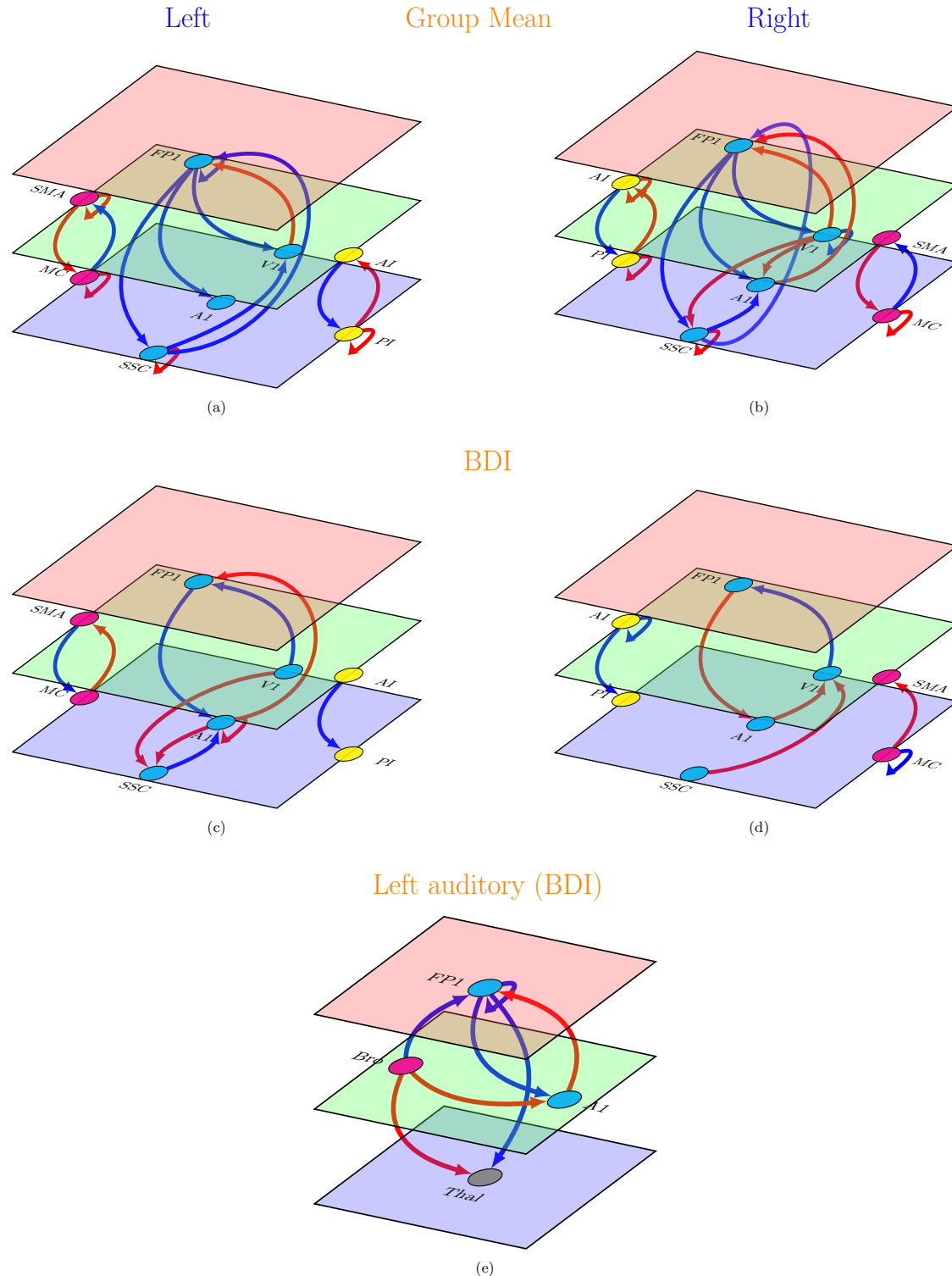
Network	Correlation	p Value
Left Motor	0.11	0.198
Left Exteroceptive	0.35	0.002
Left Interoceptive	-0.08	0.720
Right Motor	0.08	0.275
Right Exteroceptive	-0.15	0.874
Right Interoceptive	0.11	0.185

In a leave-one-out cross-validation, among all six networks, the left exteroceptive network was found to predict BDI scores at a significant level of  $\alpha = 0.05$  (see Table 1). When individual connections were considered, three connections of left exteroceptive network, namely left V1 to FP1 (corr=0.23, p-value=0.036), left A1 to SSC (corr=0.22, p-value=0.045), left SSC to A1 (corr=0.23, p-value=0.03) were found to have significant predictive power for BDI scores. Note that these measures of effect size correspond to out of sample measures (i.e., the effect sizes one would see using effective connectivity estimates from new participants).

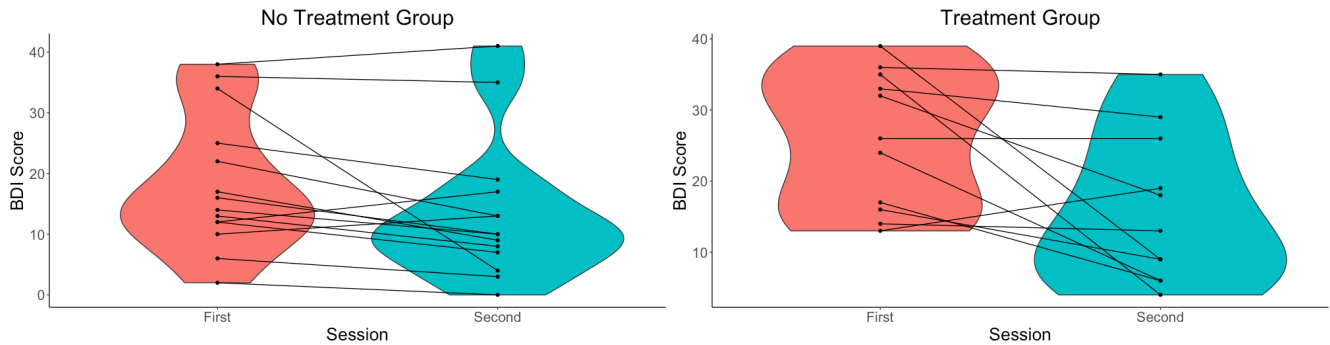
### The follow-up experiment.

**Accuracy of DCM model estimation.** As in primary analyses, the accuracy of DCM predictions for individual participants was excellent for the follow up study. The minimum percentage variance-explained by DCM model estimation across participants were 57.14%, 76.90%, and 73.33% for left motor, exteroceptive, and interoceptive networks and 76.02%, 68.70%, and 44.06% for right motor, exteroceptive, and interoceptive networks. For most of the participants variance explained was 80% or more.

**Change in BDI scores.** The BDI scores of participants during the first and the second sessions are plotted in Figure 2. As evident from the figure, for most of the participants in the treatment as well as no treatment group, BDI scores improved with time; however, improvement was more prominent in the treatment group. This was also corroborated by statistical testing. The paired samples Wilcoxon test indicated that BDI scores during the first session were statistically significantly higher than the second session for both groups at significance



**Fig. 1.** Effective connectivity in the primary study (left and right hemispheres). (a),(b): Group mean effective connectivity in sensory and motor networks. Arrow colours code nature of connections red, excitatory; blue, inhibitory. (c),(d): Connections showing significant association with Beck depression inventory (BDI) scores in sensory and motor networks. Arrow colours code direction of connectivity changes relative to the group mean: red, increased; blue, decreased. (e): Connections showing significant association with Beck depression inventory (BDI) scores in a network composed of left thalamus, left primary auditory cortex, Broca's region and left lateral frontal pole. For all subfigures line thickness is kept constant and does not code for the effect size. For the exact values of the estimated connectivity parameters see supplementary Figure 1. Colours of the planes denote position of the node in cortical hierarchy. Green is higher than blue, red is higher than both blue and green. SMA: supplementary motor area, MC: primary motor cortex, FP1: lateral frontal pole, V1: primary visual cortex, A1: primary auditory cortex, SSC: primary somatosensory cortex, AI: anterior insula, PI: posterior insula. Bro: Broca's region. Thal: Left thalamus. The images were created using tikz-network (<https://github.com/hackl/tikz-network>) package in L<sup>A</sup>T<sub>E</sub>X.



**Fig. 2.** Violin plots of the Beck depression inventory (BDI) scores in (a) no treatment and (b) treatment groups across sessions. A violin plot is a box plot with the width of the box proportional to the estimated density of the observed data.

level  $\alpha = 0.05$ . However, at significance level  $\alpha = 0.01$ , this held true only for the treatment group ( $p$ -value = 0.009491) but not for the no treatment group ( $p$ -value = 0.01176).

**Effective connectivity.** Results are displayed in Figure 3 and are further detailed in supplementary Figure 2.

**Group mean effective connectivity:** Overall, the main pattern of mean effective connectivity was reproduced by the follow up analysis. The backward connections in exteroceptive and interoceptive cortices are inhibitory and forward connections are excitatory. The opposite pattern was observed in bilateral motor cortices.

**Changes in effective connectivity with BDI scores:** Like mean effective connectivity, the changes in effective connectivity between hierarchical cortical regions with increasing depression severity follow the same pattern found in the primary analysis: with increasing BDI scores the top-down and bottom-up mean effective connectivity is enhanced in the interoceptive network and is diminished in exteroceptive and motor networks.

**Changes in effective connectivity with treatment:** With treatment, top-down and bottom-up effective connectivity revert towards group mean levels, i.e., in the exteroceptive network, top-down effective connections become more inhibitory and bottom-up connections becomes more excitatory; whereas in the motor network top-down connections became more excitatory. In the interoceptive network, no change in top-down or bottom-up effective connectivity survived at the 95% threshold set for the posterior probability of the estimated parameters.

### Cross Validation

**Table 2. leave-one-out cross validation: results from the follow-up study**

Network	Correlation	p Value
Left Motor	-0.19	0.812
Left Exteroceptive	-0.09	0.665
Left Interoceptive	0.17	0.211
Right Motor	0.15	0.237
Right Exteroceptive	-0.02	0.540
Right Interoceptive	-0.17	0.795

In a leave-one-out cross-validation, none of the effective connections were found to predict BDI scores at a significant level of  $\alpha = 0.05$  (see Table 2).

## Discussion

Overall, the most exciting findings from our study are the average backward (top-down) and forward (bottom-up) effective connectivity in sensory and motor cortices that showed consistent patterns across hemispheres and sessions and consistent changes with depression severity and treatment. The backward effective connections in exteroceptive and interoceptive sensory networks were predominantly inhibitory in nature while forward connections were predominantly excitatory (except SSC to FP1 connections in primary experiment). The opposite pattern was observed in bilateral motor networks. With increased depression scores, this pattern is weakened in exteroceptive and motor networks and is strengthened in the interoceptive network. Interestingly, with treatment, a partial recovery towards the group average was observed. In leave-one-out cross validation analysis, connections in left exteroceptive networks were found to have sufficiently large effect size to predict whether somebody has a high or a low BDI score.

There is a growing recognition that the depression is associated with dysfunction of distributed brain networks rather than of individual brain regions (44, 45). Four networks have been the focus of most of the published research in this area: the affective network (AN), reward network (RN), default mode network (DMN), and cognitive control network (CCN). Hyperconnectivity among the regions of AN (12, 14) and DMN (6, 10, 13, 16, 46) has been consistently reported in depression. Enhanced resting state functional connectivity in AN and DMN has been postulated to be associated with negative affectivity and maladaptive rumination in depression patients. Hypoconnectivity in RN (7, 17, 18) and CCN (9, 11, 47) has been another consistent finding in depression (but also see (8, 48) for divergent findings). Anhedonia and ineffective cognitive control over emotional processing seen in depression have been attributed to diminished interactions among the regions of RN and CCN, respectively.

As evident from above, the affective and psychological components of depression have been the prime focus of neurobiological research on depression. Yet, several sensorimotor interventions including light, music, tone, physical exercise are well known to modulate mood and depressive symptoms (49). Association of depression with visual (50, 51) or hearing impairment (52–54) is also well established. Depression, in turn, gives rise to several sensorimotor alterations. Some of them, for instance, psychomotor retardation or agitation and feelings





of fatigue are part of the diagnostic criteria for depression (55). Besides, there is a repertoire of subjective feelings that depressed patients experience. These include pain in several parts of the body, chest discomfort, feeling cold or nauseous, heaviness of limbs, feeling of emptiness, to mention a few (56). These feelings change the subjective experience of one's own body and one's sense of relatedness with the world outside.

There are only a few neuroimaging studies that independently examined functional connectivity in sensory and motor networks as biomarkers for depression. Among them, one recent study (57) found reduced within and between-network functional connectivity in auditory and visual networks associated with depression. In another study, Kang et al. (58) demonstrated that the primary somatosensory area-thalamic functional connectivity is abnormal in major depressive disorder. Moreno-Ortega et al. (59) showed that including resting state functional connectivity within the visual network in the analysis greatly increases the predictive power for the treatment response to electroconvulsive therapy in depression compared to model consisting of only AN and DMN.

However, our understanding of neuronal mechanisms underlying sensory perception is going through a major shift. There is an emerging consensus that perception is not a passive 'bottom-up' mechanism of progressive abstraction from sensory input and both bottom-up and top-down connectivity between hierarchically organized brain regions play crucial roles in perception. This recognition has led to several theoretical frameworks highlighting the importance of top-down information flow in the context of sensory perception. The most prominent of them - predictive coding (35-37) - has also been extended to motor function (see active inference (38)). These novel insights motivated us to analyse effective connectivity among hierarchical brain regions in sensory and motor cortices. In contrast to data-driven approaches (e.g., functional connectivity analyses) mentioned above, ours is a model-based approach informed by theoretical frameworks and empirical knowledge of functional architectures. In motor regions we chose primary motor area and supplementary motor area. The later is responsible for planning complex movements of the contralateral extremities and is posited to occupy a higher level of hierarchy in the motor system. Similarly, in interoceptive cortex we chose posterior and anterior insula based on known role of the insula in interoception and a posterior to anterior hierarchical organization in the insula (60, 61). For exteroception, we selected three primary sensory cortices: visual, auditory, and somatosensory and the lateral frontal pole - the terminal relay station for exteroceptive sensory information (62, 63).

A consistent and intriguing finding from our study is top-down inhibitory and bottom-up excitatory average effective connectivity in sensory cortices; a pattern that reverses in motor cortices. The pattern in sensory cortices is consistent with the role of top-down predictions explaining away prediction errors at lower levels, via interactions with inhibitory interneurons in canonical microcircuits (as proposed by the predictive coding framework). In other words, although long-range connections in the brain are excitatory (i.e., glutamatergic), backward connections may preferentially target inhibitory interneurons in superficial and deep layers to evince an overall decrease in neuronal message passing. In predictive coding, this is often read as 'explaining away' prediction errors at lower

levels in sensory cortical hierarchies (64). However, the completely opposite pattern was observed in the motor network. Descending excitatory connections in the motor system may reflect one of two things. First, it could be a reflection of the fact that ascending prediction errors in the executive motor system may play a small role - because these prediction errors are thought to be resolved through cortical spinal reflexes; i.e., through action (38). Put simply, in sensory hierarchies exteroceptive prediction errors are caused by bottom-up sensory input, which are resolved by (inhibitory) top-down predictions. Conversely, in motor hierarchies prediction errors are generated by (excitatory) top-down proprioceptive predictions, which are resolved by motor reflexes at the level of the spinal-cord. An alternative explanation is that descending predictions include predictions of precision that may mediate things like attention and sensory attenuation (65-67). In this instance, there can be an explaining away of certain prediction errors, while there precision may be increased, resulting in an overall excitatory drive. In other words, some descending predictions may be of proprioceptive gain that mediates the selection of intended movements. In this context it is noteworthy that descending predictions of precision play an important role in active inference accounts of psychiatric conditions - in which the synaptic pathophysiology and psychopathology can be accounted for by a failure of sensory attenuation; namely, the attenuation or suspension of the precision of sensory prediction errors. This failure of attention and attenuation has been used to explain several conditions, including autism, schizophrenia, Parkinson's disease and depression (68-72). The current results are particularly prescient in relation to formulations of depression and mood disorder in terms of active inference; namely, how actions are selected by inferring 'what to do next'. Clark, Watson and Friston (71) review the evidence for depression as a computational pathology in the proprioceptive and interoceptive (behavioural and autonomic) domain. They conclude "emotional states reflect the precision associated with neurobiological predictions over interoceptive states". The current results are consistent with this formulation but draw special attention to proprioceptive predictions in the sensorimotor system. In this setting, the attenuation of descending effective connectivity - to the executive motor cortex with increasing depression severity - is consistent with a failure to deploy sensorimotor precision appropriately during action selection. In turn, this is consistent with a failure to form precise (subpersonal) beliefs about 'what to do next', at higher levels in the sensorimotor hierarchy. An extreme example of the ensuing psychomotor poverty may be the bradykinesia of Parkinson's disease, which has a clear neuromodulatory (dopaminergic) aetiology. Please see (73) for further discussion.

In line with the marked consistency of the patterns of average effective connectivity - across hemispheres and sessions - the changes in effective connectivity with depression severity were also conserved across sessions and corroborate well with depressive symptomatology. Instead of categorically dividing participants into patients and neurotypical subjects, we examined (across participants) variation of effective connectivity with depression severity as assessed by the Beck Depression Inventory. This leverages the heterogeneity within each group that might contain useful clinical information (74). With increasing depression severity, the patterns found in top-down and bottom-up connections at the group level are weakened

349 in exteroceptive (except the left auditory cortex-see below) 410  
350 and motor cortices and strengthened in the interoceptive cortex. 411  
351 Depreciation in exteroceptive networks is in line with 412  
352 the reduced visual contrast sensitivity (20) and impaired auditory 413  
353 processing of non-speech stimuli (21). Psychomotor 414  
354 poverty or retardation is a prominent feature of depression 415  
355 (24) that might well be reflected in the weakening of motor 416  
356 network effective connectivity. The enhancement in the interoceptive 417  
357 network is consistent with increased interoceptive 418  
358 (e.g., pain) sensitivity (22) in depression. On the contrary, a 419  
359 few studies reported a subtle but non-significant association 420  
360 of depression with decreased interoceptive awareness like reduced 421  
361 heartbeat perception accuracy (75, 76). However, small 422  
362 sample sizes and/or inclusion of individuals with mild or comorbid 423  
363 presentations of depression may undermine this claim 424  
364 (77, 78). Moreover, Pollatos, Traut-Mattusch, Eva and Rainer 425  
365 (23) found that a negative relationship between depression 426  
366 and heartbeat perception accuracy is only present in those 427  
367 with relatively higher trait anxiety. Thus, it might reflect an 428  
368 interaction of anxiety with depression. Furthermore, Dunn, 429  
369 Dalgleish, Ogilvie and Lawrence (79) found that heartbeat 430  
370 perception accuracy was affected in mild depression but, paradoxically, 431  
371 was not affected in more severely depressed group thus further 432  
372 complicating the association.

373 One notable exception - to general pattern of changes in 433  
374 effective connectivity within exteroceptive network with BDI 434  
375 scores - was found in left auditory regions. Here top-down 435  
376 inhibitory and bottom-up excitatory influences were enhanced 436  
377 with depression. One possible explanation is that this reflects 437  
378 enhanced rumination and self-speech in depression; noting that 438  
379 left auditory cortex is specialized for speech perception 439  
380 (80). Rumination is implicated in the development, severity 440  
381 and maintenance of depression and other psychiatric disorders 441  
382 (81–83). Given the central role of rumination in depression, 442  
383 it has been considered a key target in modern cognitive and 443  
384 behavioural therapies (84). One of the most salient features of 444  
385 rumination is that it is mostly expressed in a verbal modality 445  
386 (85–87). In other words, while ruminating, we are mostly 446  
387 talking to ourselves silently. Thus, enhancement of effective 447  
388 connectivity within auditory network, with increasing BDI 448  
389 scores, might reflect depressive rumination during the acquisition 449  
390 of resting-state scans. To further probe this hypothesis 450  
391 we implemented spectral DCM effective connectivity analysis 451  
392 among left thalamus, Broca's area, left A1 and left FP1 452  
393 regions. Broca's area, also known as the left inferior frontal 453  
394 gyrus (LIFG), is involved in production of both outer and inner 454  
395 speech (e.g., (88)). We hypothesized that if the change in 455  
396 the pattern of effective connectivity with increasing depression 456  
397 severity is associated with rumination, left auditory area (A1) 457  
398 would be driven mainly by Broca's area. Conversely, if it 458  
399 reflects some form of aberrant sensory processing, left thalamus 459  
400 will be main driver of left A1 (89). DCM analysis demonstrated 460  
401 that with increasing BDI score effective connectivity from left 461  
402 Broca's area to left A1 becomes more excitatory but there is 462  
403 no significant change in effective connectivity from left Thalamus 463  
404 to left A1, thus providing an indirect support for the rumination 464  
405 hypothesis. It is noteworthy here that a previously published 465  
406 report of the same data found that the independent component - 466  
407 representing the left auditory network - also included the insular 467  
408 cortex in the depression group but not in the healthy participants. 468  
409 Based on several lesion

(90–94) and neuroimaging (95, 96) studies, the left insula has 410  
been proposed as a brain region involved in motor control of 411  
speech production including pre-articulatory motor responses 412  
(97–99). This lends further support to depressive rumination 413  
conjecture. 414

415 The model comparison discussed above furnishes clear evidence 416  
417 for changes in a number of extrinsic (between region) and 418  
419 intrinsic (within region) connections that underwrite depression, 420  
421 as scored with the BDI. One might ask whether these changes can 422  
423 be used diagnostically in individual patients. In other words, 424  
425 are the underlying effect sizes sufficiently large to predict whether 426  
427 somebody has a high or a low BDI score. This question goes 428  
429 beyond whether there is evidence for an association and addresses 430  
431 the utility of connectivity phenotyping for personalised medicine. 432  
433 One can address this using out of sample estimates of the effect 434  
435 size using cross validation under a parametric empirical Bayesian 436  
437 scheme (41). In other words, one can establish the predictive 438  
439 validity by withholding a particular subject and ask whether one 440  
441 could have predicted the BDI score given the effective connectivity 442  
443 estimates from that subject. This question can be posed at the 444  
445 level of a single connection or sets of connections. For example, 446  
447 when looking at single connections, three connections in the left 448  
449 hemisphere all showed a significant out of sample correlation with 450  
451 BDI score. This suggests that a nontrivial amount of variance in 452  
453 the BDI score could be explained by effective connectivity. This 454  
455 variance explained increased when considering the left exteroceptive 456  
457 network – attaining a correlation coefficient of 0.35 or, an R-squared 458  
459 of about 10% (which was extremely significant  $p < 0.001$ ). 460  
461 Although relatively small from a psychological perspective, this is 462  
463 almost an order of magnitude greater than the variance can be 464  
465 explained by genomic phenotypes (100, 101). 466

467 Clinicopathological significance of effective connectivity in 468  
469 sensory and motor cortices is further supported by the DCM 469  
470 analysis of treatment-associated changes in connectivity in the 470  
471 follow up study. Several top-down and bottom-up connections 471  
472 in bilateral exteroceptive and motor cortices were found to be 472  
473 associated with treatment. More importantly, the parity of these 473  
474 connections is opposite to the connections showing an association 474  
475 with depression severity, suggesting a prognostic relevance of 475  
476 these connectivity measures. Remarkably, none of the feedforward 476  
477 or feedback connections in the interoceptive cortex was found 477  
478 to be associated with treatment, but the clinical significance of 478  
479 this finding is unknown. Taken together, the patterned alterations 479  
480 in bidirectional connectivity with BDI scores and treatment offer 480  
481 a strong case for effective connectivity in sensory and motor 481  
482 cortices as a biomarker for depression. 482

483 A few words on the computational method used in the current 483  
484 work. DCM was introduced originally to model neuronal responses 484  
485 to external perturbation (e.g., sensory stimulation or task 485  
486 demands). DCM for resting state fMRI was subsequently introduced 486  
487 in Stochastic DCM (102). Stochastic DCMs differ from deterministic 487  
488 DCMs by allowing for physiological noise due to endogenous 488  
489 stochastic fluctuations in neuronal and vascular responses, known 489  
490 technically as system or state-noise. The opportunity to model 490  
491 endogenous (autonomous) fluctuations opened the door to identify 491  
492 the functional architectures (effective connectivity) subtending 492  
493 endogenous fluctuations observed in resting-state studies. A more 493  
494 efficient approach for resting state data was subsequently introduced 494  
495



471 which is based on fitting observed complex fMRI cross spectra (39) (For more details see Materials and Methods). This  
472 later approach, known as spectral DCM, was employed in the  
473 present study.  
474

475 Findings from the current study should be appreciated  
476 within the context of certain limitations. Although our study  
477 sample was modestly large for neuroimaging measures - and  
478 we undertook steps like cross-validation and replication of the  
479 main results to ensure the generalizability of our findings -  
480 replication in an independent sample would be an important  
481 next step. Secondly, in the context of connectivity analysis,  
482 there are several potential confounding factors other than  
483 age and sex of the participants that we have not controlled  
484 for. For example, level of anxiety in individuals could affect  
485 top-down information flow in the brain (103). Anxiety is  
486 also a common comorbidity found in depression patients (104).  
487 None of our participants reported to be diagnosed with anxiety  
488 disorders. However, the presence of subclinical anxiety was  
489 not ruled out or controlled for. We will consider testing  
490 for the association of anxiety with effective connectivity in  
491 sensory and motor networks in a companion paper. A third  
492 limitation of our study is that the analysis relied solely on  
493 BDI scores of depression. There are a large number of rating  
494 scales for assessing depression severity: some are observer  
495 rating scales, for example the Hamilton Depression Rating  
496 Scale (HDRS) and the Montgomery-Åsberg Depression Rating  
497 Scale (MADRS), others are self-rating scales (for example BDI).  
498 Each scale has its own advantages and limitations (105). Thus,  
499 the present neuroimaging findings could be further validated  
500 with a combination of observer rating scales and objective  
501 behavioural measures of depression (e.g. (106)).

502 In summary, our results advance our mechanistic under-  
503 standing of depression pathophysiology. Traditional accounts  
504 of depression (e.g. Beck's (107) cognitive model) have ne-  
505 glected bodily symptoms (79). The present work re-establishes  
506 depression as an embodied phenomenon by demonstrating that  
507 effective connectivity in sensory and motor cortices affords a  
508 promising neural signature of depression. It also establishes  
509 the generalizability and predictive validity of this novel marker  
510 - and may portend a new avenue of research into the neural  
511 underpinnings and therapeutic interventions of depression and  
512 other mental health conditions.

## 513 Materials and Methods

514 **Participant characteristics.** Fifty-one adult patients (mean age: 32.78  
515 years, SD: 8.89, 38 females, 13 males) with a diagnosis of mild de-  
516 pressive episode or moderate depressive episode according to ICD-10  
517 and twenty-one adult individuals (mean age: 33.8 years, SD: 8.5,  
518 15 females, 8 males) with no history of neurological or psychiatric  
519 illness participated. Depressed participants were either referred  
520 by a qualified psychiatrist or invited through advertisement in a  
521 popular local newspaper and then assessed by the same psychiatrist.  
522 Inclusion criterion were first diagnosed mild or moderate depres-  
523 sive episode and age between 18 and 55 years. Exclusion criteria  
524 were: previous depressive episodes, bipolar depression, seasonal  
525 depression, depression secondary to other psychiatric or somatic  
526 condition, serious risk of suicide, serious neurological and psychi-  
527 atric comorbidities, alcohol or other substance abuse or dependence,  
528 lifetime history of psychotic disorders, contraindications to MRI,  
529 extremely impaired vision, IQ score below 70, any psychotropic  
530 medication (including antidepressants), and any medication alter-  
531 ing blood pressure (that could influence fMRI signal). Healthy  
532 participants were volunteers recruited by word of mouth or via  
533 advertisement in social networks. Inclusion and exclusion criteria

534 for healthy volunteers were the same, except for the presence of  
535 depressive episodes. The depressed and neurotypical participants  
536 did not differ in level of intelligence (mean (SD) Raven's Progressive  
537 Matrices test score, for neurotypicals: 105.9(16.5), for depression  
538 patients: 103.7(14.6)). All participants gave informed consent in  
539 accordance with the Declaration of Helsinki. Ethical review board  
540 of Research Institute of Molecular Biology and Biophysics approved  
541 the study. Beck depression inventory evaluation could not be done  
542 on four patients and three neurotypical participants. Consequently,  
543 sixtyfive participants were included in the final analysis.

544 Twenty-nine depression patients from the primary study were  
545 included in the follow-up study ( gap between two sessions, minimum:  
546 56 days, maximum: 234 days). Among them fifteen individuals  
547 received no treatment, eight received cognitive behavioural therapy  
548 (CBT) and six received neurofeedback therapy (NFBT). BDI scores  
549 could not be retrieved for one participant during the first scan  
550 and for four participants during the second scan and subsequently  
551 twenty-four participants were included in the final analysis. We  
552 checked for systemic differences between participants who attended  
553 both the sessions and who dropped out. A Mann-Whitney test  
554 failed to show between-group differences in age, IQ, and emotional  
555 variables at a significance level of 0.05. At the same significance level,  
556 the chi-square analyses failed to show significant differences between  
557 two groups in terms of sex ratio and mild/moderate depression  
558 ratio.

559 It is noteworthy here, data from a subset of participants from  
560 the present study has been published (46, 108, 109). However, those  
561 works mainly employed a data-driven approach based on indepen-  
562 dent component analysis (ICA) decomposition of the whole-brain  
563 data and correlation based (undirected) functional connectivity  
564 analysis unlike the current study that tests a specific hypothesis  
565 by investigating (directed) effective connectivity in functionally  
566 characterised brain regions.

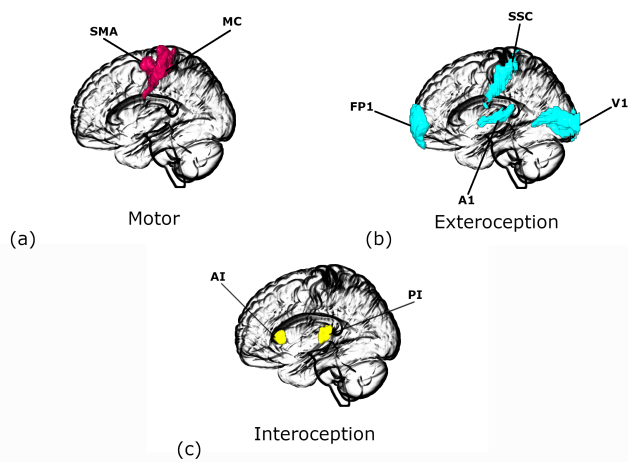
567 **Brain MRI acquisition.** The fMRI acquisition was carried out in the  
568 International Tomography Center, Novosibirsk. Imaging data were  
569 acquired with an Ingenia (Philips) 3T scanner using a 32-channel  
570 dStream HeadSpine coil (digital). The structural and functional  
571 images had the following parameters:  
572 Structural MRI: T1 3D TFE, Field of View:  $250 \times 250 \times 280 \text{ mm}^3$ ,  
573 TR/TE=7.5/3.7 ms, Flip Angle=  $8^\circ$ , Voxel size:  $1 \times 1 \times 1 \text{ mm}^3$ .  
574 Functional MRI: T2\* Single shot SPIR EPI, Field of View:  
575  $220 \times 220 \text{ mm}^2$ , TR/TE=2500/35 ms, Flip Angle=  $90^\circ$ , Voxel size:  
576  $2 \times 2 \times 5 \text{ mm}^3$ , 25 slices.

577 During the resting state sequence (duration: four minutes each),  
578 participants were instructed to lie still and motionless in the scanner  
579 with their eyes closed while letting their mind wander.

580 **Preprocessing.** The pre-processing and statistical analysis of fMRI  
581 data were executed with the SPM12 v7771 toolbox (Statistical Para-  
582 metric Mapping, <http://www.fil.ion.ucl.ac.uk/spm>). The initial five  
583 scans were discarded to allow the magnetization to stabilize to a  
584 steady state. Prior to statistical analysis, images were slice-time  
585 corrected, realigned with the mean image, motion corrected, coreg-  
586 istered with the corresponding T1-weighted images, normalized to  
587 a Montreal Neurological Institute (MNI, <https://www.mcgill.ca>)  
588 reference template and resampled to  $4 \times 4 \times 5 \text{ mm}^3$ . During mo-  
589 tion correction, 2nd-degree B-Spline interpolation was used for  
590 estimation and 4th-degree B-Spline for reslicing. Coregistration  
591 used mutual information objective function while normalization used  
592 4th-degree B-Spline interpolation. Images were smoothed with a full-  
593 width at half-maximum (FWHM) Gaussian kernel  $4 \times 4 \times 10 \text{ mm}^3$   
594 and further denoised by regressing out several nuisance signals,  
595 including the Friston-24 head motion parameters and signals from  
596 cerebrospinal fluid and white matter. Temporal high pass filtering  
597 above 1/128 Hz was employed to remove low-frequency drifts caused  
598 by physiological and physical (scanner related) noises.

599 **Spectral Dynamic Causal Modelling and Parametric Empirical Bayes.**  
600 The Spectral DCM approach using DCM12.5 as implemented in  
601 SPM12 v7771 (<http://www.fil.ion.ucl.ac.uk/spm>) was used to es-  
602 timate the effective connectivity within each network. Dynamic  
603 causal modelling (DCM) is Bayesian framework that infers the  
604 causal architecture of distributed neuronal systems from the ob-  
605 servable BOLD (blood-oxygen-level-dependent) activity recorded





**Fig. 4.** Regions of interest for (a) Motor, (b) Exteroceptive, and (c) Interoceptive networks. SMA: supplementary motor area, MC: primary motor cortex, FP1: lateral frontal pole, V1: primary visual cortex, A1: primary auditory cortex, SSC: primary somatosensory cortex, AI: anterior insula, PI: posterior insula. The images were created using MRICroGL (<https://www.nitrc.org/projects/mricrogl/>) program.

Time series for DCM analysis were extracted for each region of interest by taking the first principal components of the time series from all voxels included in the masks for that region. Masks were defined according to SPM Anatomy toolbox (114). The regions of interest for each network are depicted in Figure 4. We also adjusted data for “effects of interest”, thus effectively mean-correcting the time series.

At the first level, fully-connected models (i.e., between all nodes plus self-loops) were estimated for each subject individually, separately for bilateral exteroceptive, interoceptive and motor networks.

A basic diagnostic of the success of model inversion is to look at the average percentage variance-explained by DCM model estimation when fitted to the observed (cross spectra) data. We implemented this diagnostic test across participants.

At the second (group) level, we used parametric empirical Bayes (PEB) — a between-subjects hierarchical Bayesian model over parameters — which models how individual (within-subject) connections relate to different between-subjects effects (41, 115) (Friston, Zeidman and Litvak, 2015; Friston et al., 2016). Unlike a classical test (e.g., t-test), it uses the full posterior density over the parameters from each subject’s DCM — both the expected strength of each connection and the associated uncertainty (i.e., posterior covariance) — to inform the group-level result. The group mean, by default, is the first regressor or covariate. In the primary study, BDI scores, age, sex are the next three regressors. Age and BDI scores were mean-centred (across all subjects) to enable the first regressor to be interpretable as the mean. In the follow up study, treatment (treatment received vs not treated) was included as the fifth regressor. To evaluate how regions in the network of interest interact, we used Bayesian model comparison to explore the space of possible hypotheses (or models). Candidate models were obtained by removing one or more connections to produce nested or reduced forms of the full model. As there is large number of possible nested models in the model space, the search algorithm used Bayesian model reduction (BMR) (41) that enables an efficient (greedy) search of the model space. BMR prunes connection parameters from the full model and scores each reduced model based on the log model-evidence or free energy. The process continues until there is no further improvement in model-evidence. The parameters of the selected models from this search procedure were then averaged, weighted by their model evidence (Bayesian Model Averaging) (116).

**Leave-one-out validation analysis.** Finally, we tested whether the severity of depression could be predicted based on the modulation of effective connectivity. In other words, was the effect size large enough to have predictive validity. We chose connections that survived a threshold of 95 % posterior probability (very strong evidence) in the previous analysis (primary study). We used a leave-one-out scheme as described in (41). A parametric empirical Bayesian model was estimated while leaving out a subject, and was used to predict the BDI score of the left out subject, based on the specific connections chosen. The Pearson’s correlation between the predicted score and known score was calculated.

**Data and code availability.** Our analysis code is available on GitHub (<https://github.com/dipanjan-neuroscience/depression2021>). Imaging data are available on OpenNeuro (<https://openneuro.org/datasets/ds002748/versions/1.0.3> & <https://openneuro.org/datasets/ds003007/versions/1.0.0>).

**ACKNOWLEDGMENTS.** We thank Prof. Mark Shtark who supervised the data collection and Dr. Andrey Savelov who conducted MRI and fMRI acquisition. This research was supported by the Basque Government through the BERC 2018-2021 program, by the Spanish Ministry of Science, Innovation, and Universities (BCBL Severo Ochoa excellence accreditation SEV-2015-0490 and BCAM Severo Ochoa accreditation SEV-2017-0718) and the project MTM2017-82379-R (AEI/FEDER,UE) (principal investigator: Dr. Maria Xose Rodriguez, BCAM). Data collection was funded by the Russian Science Foundation grant #16-15-00183. K.J.F. was funded by a Wellcome Trust Principal Research Fellowship (Ref: 088130/Z/09/Z).

in fMRI. It is primarily based on two equations. First, the neuronal state equation models the change of a neuronal state-vector in time, depending on modulation of connectivity within a distributed system and experimental perturbations. Second, an empirically validated hemodynamic model that describes the transformation of neuronal state into a BOLD response. For task fMRI, external stimuli usually forms the external perturbation component. For resting-state fMRI, in the absence of external stimuli — a stochastic component capturing neural fluctuations is included in the model and the neural state equation can be represented as

$$\dot{x}(t) = f(x(t), \theta) + v(t) \quad [1]$$

where  $\dot{x}$  is the rate of change of the neuronal states  $x$ ,  $\theta$  represents unknown parameters (i.e., intrinsic effective connectivity) and  $v(t)$  is the stochastic process modelling the random neuronal fluctuations that drive the resting-state activity. The observation equation could be written as:

$$y(t) = h(x(t), \phi) + e(t) \quad [2]$$

Here,  $y(t)$  is the observed BOLD activity,  $\phi$  are the unknown parameters of the (haemodynamic) observation function, and  $e(t)$  is the stochastic process representing the measurement or observation noise.

Spectral DCM offers a computationally efficient inversion of the stochastic model for resting state fMRI. Spectral DCM simplifies the generative model by replacing the original BOLD time-series with their second-order statistics (i.e., cross spectra). This allows circumventing estimation of time varying fluctuations in neuronal states by estimating their covariance, which is time invariant. In other words, the problem of estimating hidden neuronal states disappears and is replaced by the problem of estimating their correlation functions of time or spectral densities over frequencies (and observation noise) where a scale free (power law) form is used (motivated from previous works on noise in fMRI (110) and underlying neuronal activity (111, 112)) as follows:

$$\begin{aligned} g_v(\omega, \theta) &= \alpha_v \omega^{-\beta_v} \\ g_e(\omega, \theta) &= \alpha_e \omega^{-\beta_e} \end{aligned} \quad [3]$$

Here,  $\{\alpha, \beta\} \subset \theta$  are the parameters controlling the amplitudes and exponents of the spectral density of the neural fluctuations. Finally, standard Bayesian model inversion (i.e. Variational Laplace) is used to infer the parameters of the models from the observed signal. A detailed mathematical treatment of spectral DCM can be found in (39) and (113).

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