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Latent functional connectivity underlying multiple brain states

Short Title: Latent functional connectivity

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46

Abstract

47 Functional connectivity (FC) studies have predominantly focused on resting state, where ongoing
48 dynamics are thought to reflect the brain's intrinsic network architecture, which is thought to be
49 broadly relevant because it persists across brain states (i.e., is state-general). However, it is
50 unknown whether resting state is the optimal state for measuring intrinsic FC. We propose that
51 latent FC, reflecting shared connectivity patterns across many brain states, better captures state-
52 general intrinsic FC relative to measures derived from resting state alone. We estimated latent
53 FC independently for each connection using leave-one-task-out factor analysis in 7 highly
54 distinct task states (24 conditions) and resting state using fMRI data from the Human
55 Connectome Project. Compared to resting-state connectivity, latent FC improves generalization
56 to held-out brain states, better explaining patterns of connectivity and task-evoked activation. We
57 also found that latent connectivity improved prediction of behavior outside the scanner, indexed
58 by the general intelligence factor (g). Our results suggest that FC patterns shared across many
59 brain states, rather than just resting state, better reflects state-general connectivity. This affirms
60 the notion of “intrinsic” brain network architecture as a set of connectivity properties persistent
61 across brain states, providing an updated conceptual and mathematical framework of intrinsic
62 connectivity as a latent factor.

63

Introduction

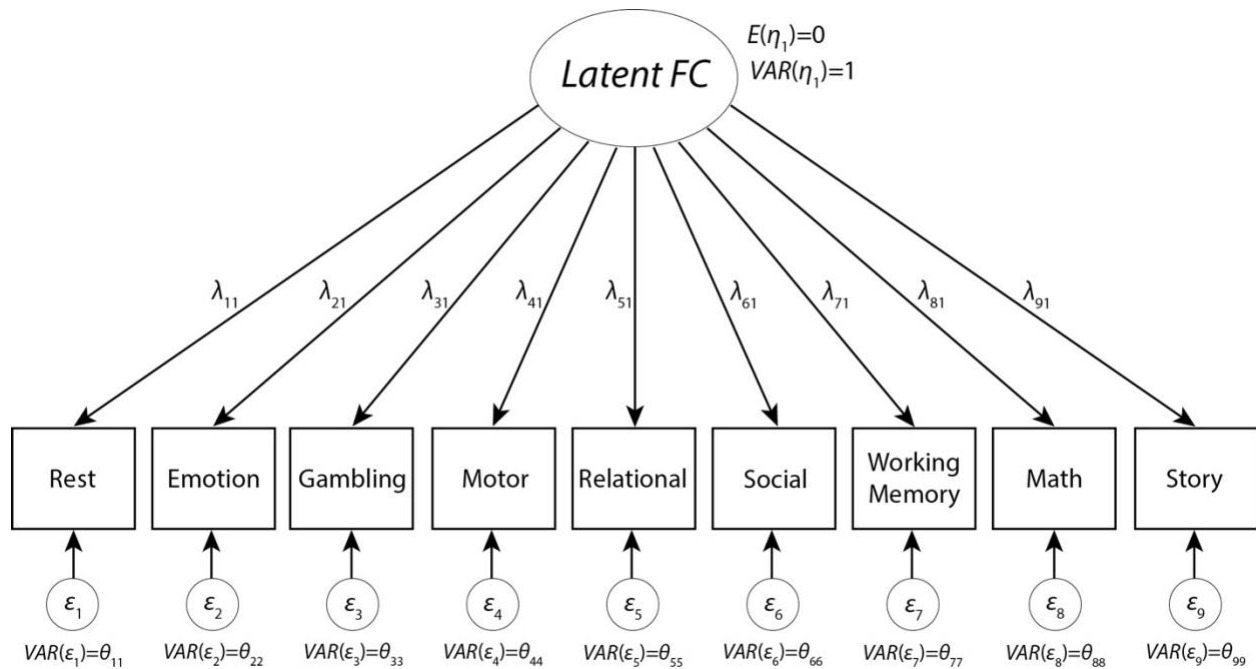
64 A major goal in cognitive neuroscience in recent years has been to move away from
65 characterizing brain activation and connectivity in specific task states towards understanding
66 “intrinsic” or context-free brain activity. Such activity reflects the more than 95% of metabolic
67 brain activity that remains unchanged across cognitive demands (Raichle, 2006). This ongoing
68 brain activity persists across states and is not attributable to external stimuli or task demands.
69 Efforts to understand intrinsic function have focused primarily on statistical associations between
70 brain activity time series (functional connectivity; FC) during the resting state (Fox & Raichle,
71 2007) (but see (Finn et al., 2015; Greene, Gao, Scheinost, & Constable, 2018) for task-based
72 investigations), which has revealed an intrinsic brain functional network architecture that
73 recapitulates patterns of task-evoked brain activity (Cole, Ito, Bassett, & Schultz, 2016; Smith et
74 al., 2009) and structural connectivity (Honey et al., 2009). As the name implies however, resting
75 state is just one state that the brain can occupy, and a truly “intrinsic” connectivity network should
76 persist across the many different states a brain might assume. In other words, a “state-general”
77 intrinsic network. Despite its importance for understanding brain function, many uncertainties
78 remain on how to best estimate intrinsic FC. While some efforts have focused on the need to obtain
79 longer resting-state scans (Anderson, Ferguson, Lopez-Larson, & Yurgelun-Todd, 2011; Elliott et
80 al., 2019; Hacker et al., 2013; Laumann et al., 2015) more recent approaches have highlighted
81 advantages of combining resting-state and task data to analyze intrinsic activity.

82 This second set of approaches leverages functional data across different task (and rest)
83 scans in order to improve the reliability of FC estimates and their predictive utility (Elliott et al.,
84 2019) Because of the relatively high stability of FC networks across task states (Cole, Bassett,

85 Power, Braver, & Petersen, 2014; Gratton et al., 2018; Krienen, Yeo, & Buckner, 2014),
86 combining data across task runs aims to distinguish what is common across a larger set of brain
87 states. What is common therefore reflects the intrinsic patterns of covariance in the brain, while
88 variation between different brain states is treated as noise in the combined data. However, this
89 work largely relies on averaging data from multiple scans together (Elliott et al., 2019). While this
90 approach has been shown to be useful, and has the advantage of simplicity, there are potential
91 theoretical limitations to such an approach that may limit its generalizability. Given its ubiquity
92 and close-formed, arithmetic solution, the average is rarely thought of as a formal statistical model.
93 However, recent work (McNeish & Wolf, 2020) has shown that the average can be thought of as
94 a restricted case of the more-general factor analytic model. Embedding the average in a
95 theoretically rich statistical framework is likely to offer advantages for interpretation of results
96 using this measure as well as insights into the measure itself.

97 Factor analysis has a long tradition in the behavioral sciences (Spearman, 1904; Thurstone,
98 1935) and is an invaluable tool in psychometrics and psychological measurement. Its key insight
99 is that observed measures (e.g., behavioral responses or fMRI scans) are imperfect manifestations
100 of an unobserved (i.e., latent) variable (Bollen, 2002). In the factor model, observed indicators ($y_{i,t}$;
101 i = individual, t = task state) are modeled as dependent on the underlying latent factor (η ; Figure
102 1). Variability in the indicators is partitioned into common variance (transmitted through the factor
103 loading matrix, Λ) and unique variance (ϵ_t). In this model, latent FC represents an unmeasured,
104 underlying brain state that is common to all observed brain states (i.e., the indicators: resting state,
105 motor task, etc.), but we also explicitly model additional variance that is only found in each
106 individual task state through the error terms. Factor loadings for the individual task states (e.g., λ_{11}

107 for Rest) in this single-factor model can be interpreted as the proportion of variance explained in
108 each task state by latent FC (similar to R^2 in regression).



109 **Figure 1. Factor Model.** A set of indicators (e.g., Rest, the Motor task, etc.) are modeled being composed of shared
110 underlying variance, as represented by the latent factor (i.e., Latent FC), and unique task-state variance (in the
111 errors). Factor loadings (λ) represent the percent variance in each task state that is explained by the underlying Latent
112 FC.
113

114

115 As can be seen in Figure 1, the factor analysis model of latent FC is a parameter-rich model
116 that allows for differentially weighted relationships between the underlying latent connectivity and
117 measured connectivity in each specific state. What McNeish and Wolf (2020) showed, however,
118 is that the average can be recovered using this model by setting all factor loadings (λ) equal to 1
119 and the unique variances to 0. This recast of the average as a special case of the factor model not
120 only has the advantage of making the assumptions of the average clearer, but it enables a formal
121 test of those assumptions. For instance, by setting all factor loadings equal, the average assumes
122 that each observed FC state is equally (and positively) related to the underlying latent FC. If we
123 want to relax that assumption, the factor analytic model can be used to compute unique optimally

124 weighted values for each factor loading, which suggests that some observed states may be better
125 (or worse) reflections of underlying latent FC. Indeed, factor loadings may take on negative values,
126 which implies that an observed indicator is anti-correlated with the underlying latent FC. However,
127 if the assumption of equal, positive weighting is indeed an appropriate assumption, freely
128 estimated factor loadings will converge towards equal values and approximate the average. In
129 other words, the flexibility of the full factor loading does not preclude the average, but instead
130 offers a broader range of possibility for deriving a measure of latent FC in heterogeneous data and
131 can be used to test the validity of the average FC assumption of equal positive factor loadings
132 across brain states.

133 Here, we test the reliability of a factor analytic framework for modeling state-general brain
134 connectivity – “intrinsic” FC that generalizes across a variety of brain states. First, we
135 hypothesized that latent FC reflects a positive manifold (analogous to the positive correlations
136 across intelligence tests in general intelligence research; (Kovacs & Conway, 2016)), where all
137 state-specific connectivity values are positively correlated with each other and so load positively
138 onto the underlying latent variable. This would confirm that a single common intrinsic functional
139 network architecture exists across conscious brain states. Importantly, this differs from the idea
140 that states are correlated (Finn et al., 2015; Gratton et al., 2018) as between-subject variance is
141 decomposed at each individual connection rather than correlating across connections. We further
142 hypothesized that by combining information across task states, such as in the factor model, a more
143 reliable measure of “intrinsic” connectivity can be estimated than when using resting state data
144 alone (the current field standard). This would suggest that resting-state FC is not necessarily the
145 best state for estimating intrinsic FC, especially if resting state does not load higher on the latent
146 variable than other states. In testing these hypotheses, we developed an analytic framework for

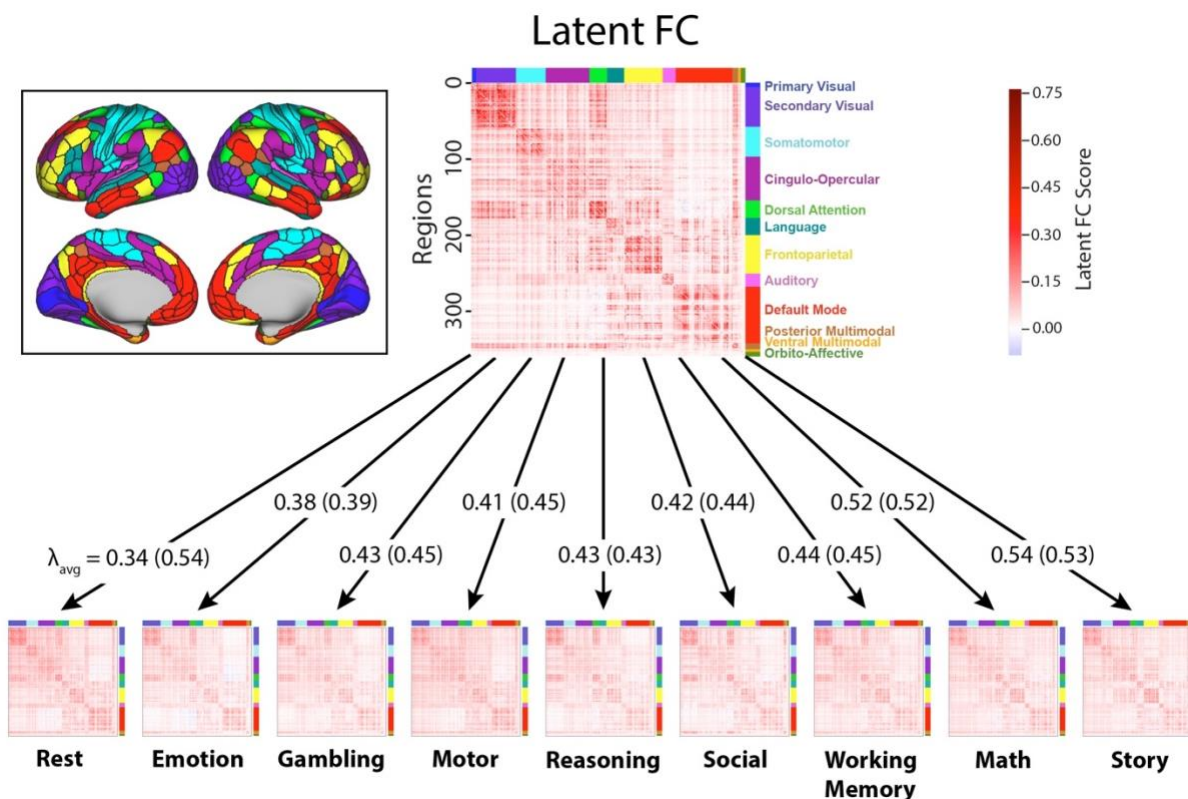
147 estimating state-general, latent FC in whole-brain functional data. Using multi-task fMRI data
148 from the Human Connectome Project (HCP), we compare the ability of latent and resting-state FC
149 to predict task-evoked activation and task-state FC for held-out brain states, as well as to explain
150 individual differences in psychometric “g” (a measure of human intelligence derived with a similar
151 factor analytic model). Results demonstrate the promise of the latent variable approach in
152 functional neuroimaging, particularly for the estimation of intrinsic FC that generalizes beyond
153 specific brain states (e.g., rest). Finally, we demonstrate the relationship between freely estimated
154 latent FC and the simpler average FC approach and discuss the theoretical advantages of casting
155 both methods in the latent variable framework for future work.

156 **Results**

157 **Factor analysis model of latent connectivity**

158 We ran independent factor analysis models for each connection, estimating the factor
159 loadings of the latent variable (i.e., latent FC) onto each state. Latent FC captures the shared
160 variance in FC across all states (see Figure 2). Factor analyses were run using all available data
161 (i.e., the full time series and all states). All analyses were performed in the exploratory sample
162 independently and then replicated in the validation sample (both $N = 176$; see the Participants
163 section for additional information). Importantly, all factor analytic models were fit for each sample
164 separately to avoid issues of circularity when comparing results across samples.

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166
167 **Figure 2. Factor analysis model of latent FC.** Visualization of the latent connectivity matrix and state-specific
168 functional connectivity matrices (group average across subjects). Color along the axes of each matrix corresponds to
169 the network membership of each ROI. For each arrow, the average loadings (λ_{avg}) for each state are shown for
170 analyses controlling for number of TRs (first) and when not controlling for TRs (in parentheses). The averaging
171 loadings for the task states were largely stable across analyses, but the average loading for resting-state increased
172 substantially (from 0.34 to 0.54) when not controlling for the number of TRs. The amount of resting-state data per
173 participant went from 4800 TRs (58 minutes) to 2112 TRs (25 minutes) when matching the total amount of “on-task”
174 time. The network mapping is shown in the cutout (left). Elements in the state-specific matrices represent correlations
175 (r) between regional time series and elements in the latent FC matrix represent factor scores computed from the model
176 for each connection.

177
178 Consistent with our hypothesis that there is a “positive manifold” demonstrating a common
179 latent FC architecture across states, almost all factor loadings were positive (greater than 99%)
180 across all connections and all states (see Table 1). Furthermore, 70.7% of all factor loadings were
181 reasonably large in magnitude (factor loading ≥ 0.4) and 97.4% of connections had two or more
182 states with factor loadings ≥ 0.4 in the full latent FC model. The emotion task had the fewest large
183 factor loadings (47.3%) and the resting state had the most (92.6%) (see Table 1 for full details).

184 To control for differences between states in the amount of data used to obtain state-specific
185 FC estimates, factor analyses were re-run while matching the number of time points from rest and

186 task data (2112 TRs from rest and 264 TRs for each of the 8 tasks). With this approach, resting
187 state had the fewest number of relatively high magnitude factor loadings of all states – only 31.6%
188 of resting state connections had factor loadings ≥ 0.4 . Thus, resting state had the highest factor
189 loadings onto latent FC when a large amount of data was used to estimate resting-state FC, but the
190 lowest factor loadings when less data was used. Controlling for the number of time points between
191 task and rest led to less pronounced changes in the factor loadings of the other states (see Figure
192 2), likely because there was no relationship between the number of TRs for a given task state and
193 its average factor loading in the full TR analysis (see Figure S1). Note that this drop occurs even
194 though rest continues to have substantially more TRs (8x) than any given task state in these
195 analyses.

State	All Data		Controlling for # Timepoints	
	% Loadings ≥ 0	% Loadings ≥ 0.4	% Loadings ≥ 0	% Loadings ≥ 0.4
Rest	99.9%	92.6%	99.0%	31.6%
Emotion	99.3%	47.3%	98.7%	46.3%
Gambling	99.6%	65.0%	99.1%	62.2%
Motor	99.8%	68.0%	99.4%	54.8%
Reasoning	99.5%	62.1%	99.1%	62.3%
Social	99.8%	66.2%	99.3%	58.4%
Working Memory	99.7%	67.0%	99.2%	64.9%
Math	99.9%	82.4%	99.6%	82.4%
Language	99.9%	86.0%	99.7%	86.3%

196 **Table 1: Factor Loadings.** Almost all factor loadings were positive regardless of whether all resting state data were
197 used (left) or we controlled for the number of time points between task and rest (right). Only resting state showed a
198 substantial shift in the percent of factor loadings ≥ 0.4 when controlling for the number of timepoints. The amount of
199 resting-state data per participant went from 4800 TRs (58 minutes) to 2112 TRs (25 minutes) when matching the total
200 amount of “on-task” time.

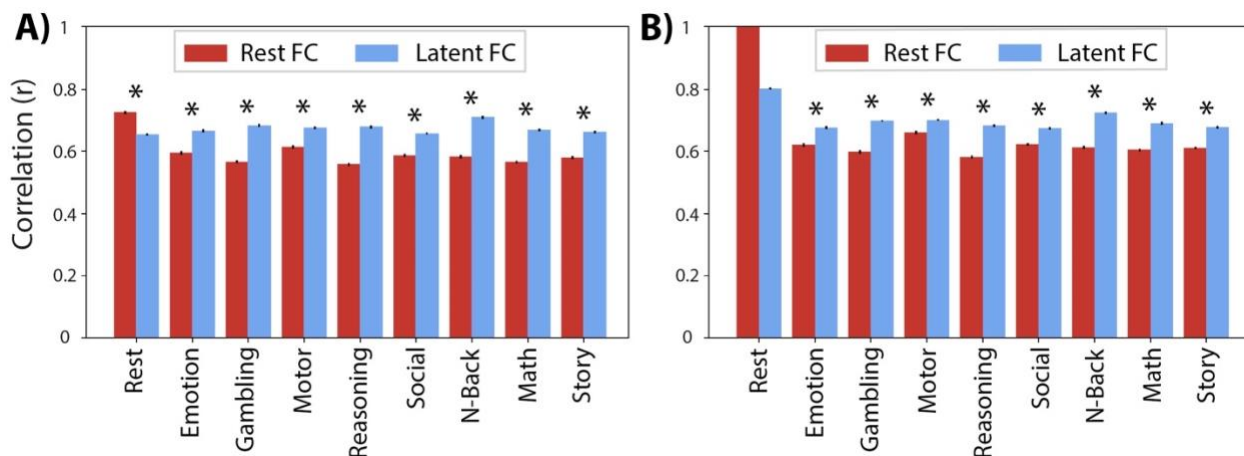
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202 **Latent FC improves generalization to connectivity of held-out states**

203 We next sought to test our second hypothesis: A more reliable and generalizable measure
204 of “intrinsic” connectivity can be estimated by combining information across task states, such as
205 in the factor model, than by using resting state data alone (the current field standard). To test
206 whether the measures of intrinsic FC persist across brain states, we quantified the
207 generalizability of rest FC and latent FC to held-out brain states. To calculate the similarity of
208 FC patterns (i.e., across 64,620 network connections), we computed the Pearson’s correlation of
209 rest FC or latent FC with state FC for each individual subject, applying Bonferroni correction to
210 correct for multiple comparisons. For latent FC, similarity was always computed for the state that
211 was held-out while running the factor analysis model. Compared to rest FC, we found that latent
212 FC exhibited significantly greater similarity with a variety of independent brain states (see
213 Figure 3A). Similarity of each state with latent FC was comparable across states, exhibiting the
214 greatest similarity to the WM task ($r = 0.71$) and the least similarity to the social task ($r = 0.66$)
215 and resting state ($r = 0.65$). Rest FC exhibited the greatest similarity to the full resting state data
216 ($r = 0.73$), providing a measure of test-retest similarity of rest FC (i.e., how well the restricted
217 TR data represents the correlation matrix computed on the complete resting state data). For the
218 task states, rest FC had the greatest similarity to the motor task ($r = 0.61$) and the least similarity
219 to the relational task ($r = 0.56$).

220 When using the full timeseries (i.e., not controlling for the amount of data used to obtain
221 the FC estimates across states), we still found greater similarity of latent FC relative to rest FC
222 with the task states. However, latent FC exhibited the greatest similarity to the resting state ($r =$
223 0.80) and the least similarity to the social task ($r = 0.67$; see Figure 3B). Alongside greater
224 similarity estimates with all states, this suggests that states may converge towards latent FC as
225 we sample substantially more data for any given state (e.g., for resting-state FC, 26 minutes of

226 data per participant were included in the data-restricted analysis vs. 58 minutes of data in the
227 unrestricted analysis). All findings were replicated in the validation dataset (Figure S2).
228



229
230 **Figure 3. Generalizability of FC patterns.** Pearson's correlation was used to quantify the similarity of latent FC
231 (blue) and rest FC (red) to held-out state FC. Error bars show the standard error of the mean. Asterisks indicate
232 significant differences in similarity of latent FC and rest FC to held-out state FC. **A)** Results when controlling for the
233 number of time points in the resting state data. This included 25 minutes of resting-state fMRI data, matching the total
234 amount of "on-task" time across all tasks. **B)** Results when not controlling for the number of time points (including
235 58 minutes of resting-state data); the resting state prediction is therefore a perfect reproduction (no error bars or
236 comparison). These results are consistent with resting-state FC overfitting to resting state, reducing its
237 generalizability relative to latent FC.

238

239 Latent FC improves prediction of task activation patterns

240 We next sought to further test our hypothesis that latent FC is highly generalizable (relative
241 to resting-state FC), this time by testing for generalization beyond FC to patterns of task-evoked
242 activation. We began by using GLMs to estimate the pattern of task-evoked activation for each of
243 24 task conditions. We then used activity flow mapping (Figure 4A) to predict the pattern of task-
244 evoked activation based on a simple neural network model parameterized using either resting-state
245 FC or latent FC. We used Pearson's correlation to compute the similarity of predicted-to-actual
246 task activations of two activity flow models with different connectivity estimates based on either
247 latent FC or rest FC. As a global measure of performance, we first correlated the predicted
248 activation patterns from the activity flow model using rest and latent FC with the observed

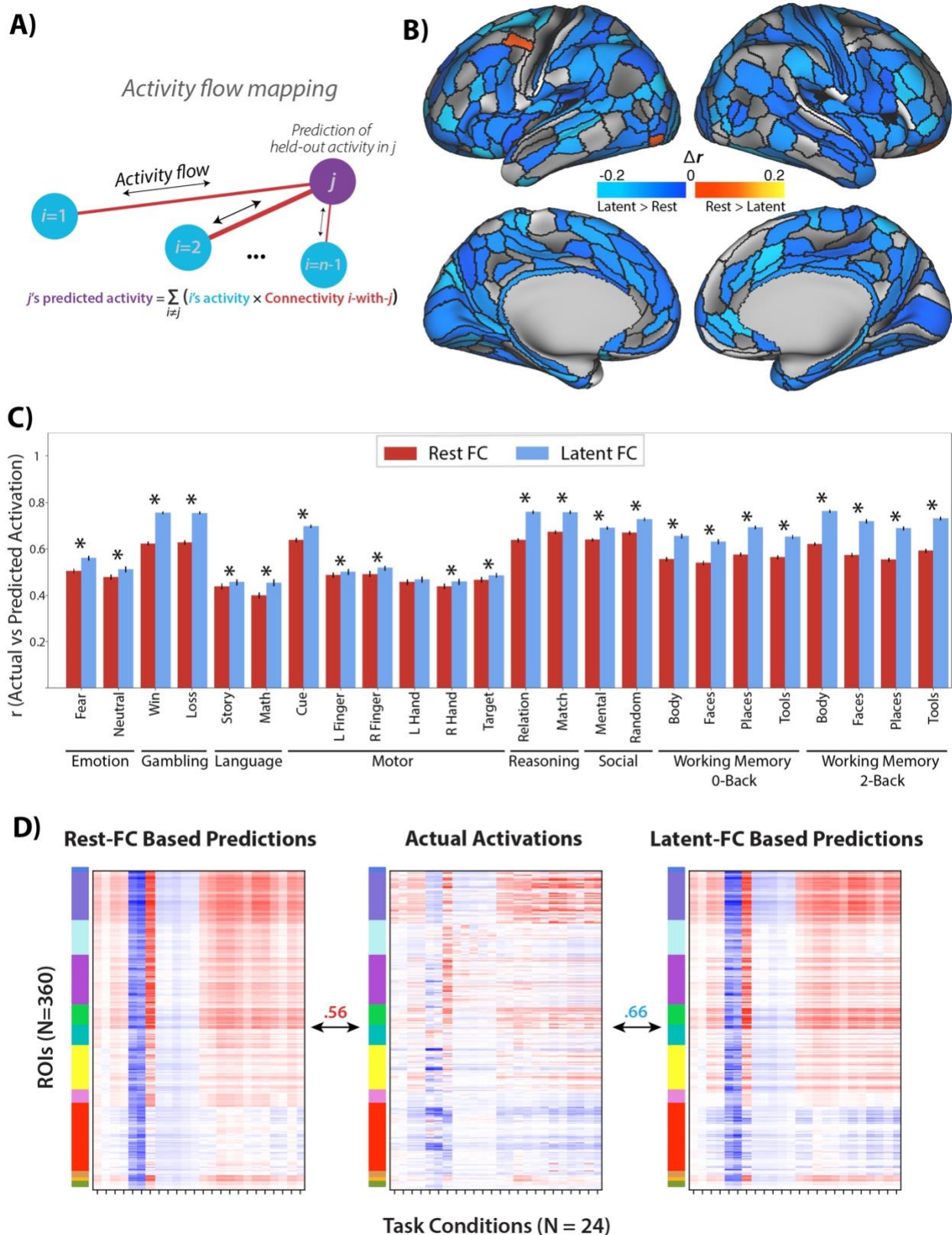
249 activations. Predicted activation patterns from activity flow models with connectivity based on
250 latent FC ($r = 0.66$) outperformed predictions based on resting state FC ($r = 0.56$) in reproducing
251 the observed beta activation patterns (Figure 4D). We then compared the results of the two models
252 at the region (i.e., prediction for a given region across conditions) and condition (i.e., prediction
253 for a given condition across regions) level.

254 We first estimated predicted beta activations for each region (across conditions) using the
255 activity flow models. This reflects the changes in activation within each region that are dependent
256 on the task condition. For each region, we compared the beta activation predictions of the two
257 activity flow models. For each network, we computed the percent of regions with significantly
258 improved predictions for one of the two models. When using the activity flow model based on
259 latent FC, the predictions were significantly improved (based on a corrected t-test of z-transformed
260 correlation coefficients) for 68% of brain regions (246 out of 360 total), accounting for 33% of
261 VIS1, 69% of VIS2, 64% of SMN, 73% of CON, 70% of DAN, 62% of LAN, 62% of FPN, 100%
262 of AUD, 78% of DMN, 14% of PMM, 0% of VMM, and 33% of ORA. Activity flow based on
263 rest FC significantly improved predictions in 1% of brain regions (4 out of 360 total), accounting
264 for 7% of VIS2 and no other networks (Figure 4B).

265 When considering prediction accuracy for each task condition, we found that latent FC
266 significantly improved the across-region predicted activations for all task conditions – except the
267 left-hand condition of the motor task – when comparing the relative activations across the topology
268 of the brain within a condition (Figure 4C). Overlap of predicted-to-actual task activations for the
269 activity flow models were variable by task condition. The activity flow model based on latent FC
270 exhibited the greatest similarity to the 2-back body condition of the WM task ($r = 0.76$) and the
271 least similarity to the math condition of the language task ($r = 0.45$). The activity flow model based

272 on rest FC exhibited the greatest similarity to the matching condition of the relational task ($r =$
273 0.67) and the least similarity to the math condition of the language task ($r = 0.4$). All findings were
274 replicated in the validation dataset (Figure S3).

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Figure 4. Comparison of activity flow models based on latent FC versus rest FC. **A)** Conceptual model of the activity flow mapping algorithm (Cole et al., 2016) which models the activity of a held-out region (j) as the sum of activity in other brain regions (i) weighted by their shared functional connectivity (ij). **B)** Task activation prediction accuracies

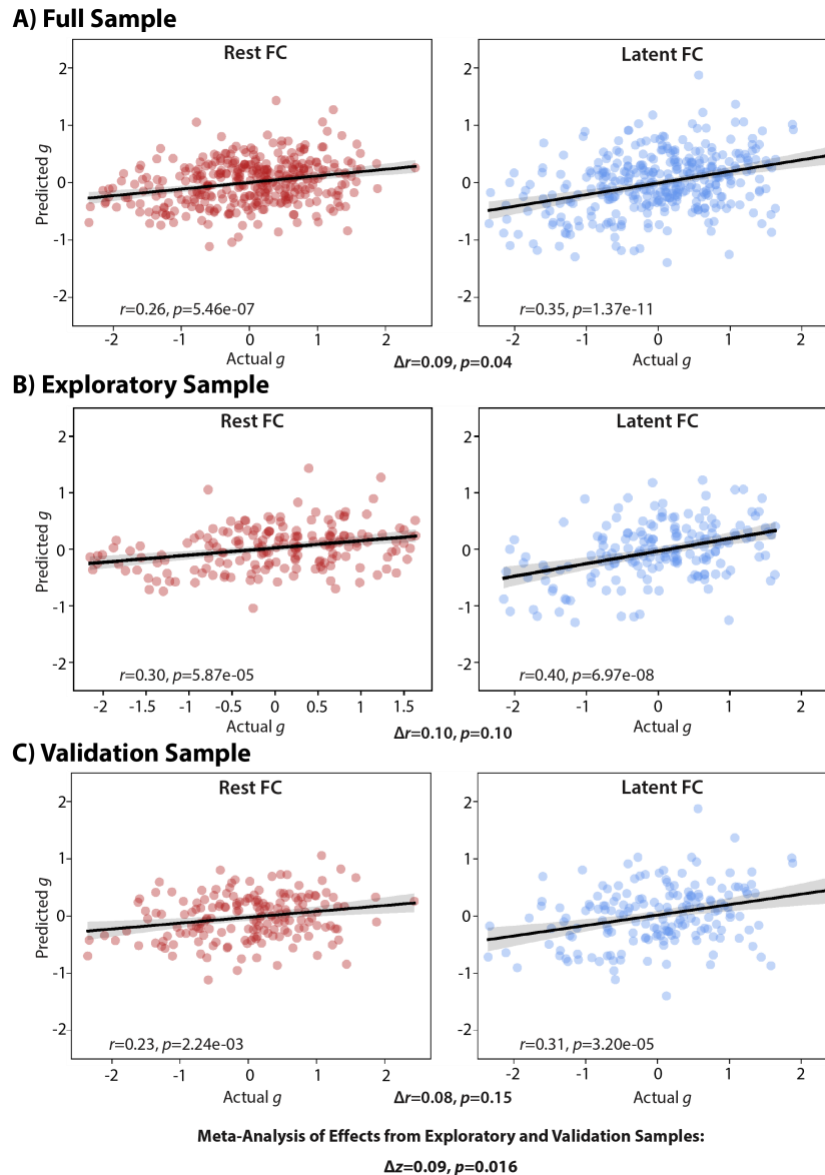
280 *by region. Regions with prediction accuracies that were significantly greater using the activity flow model based on*
281 *latent FC shown in cool colors. Regions with prediction accuracies that were significantly greater using the activity*
282 *flow model based on rest FC shown in warm colors. The vast majority of regions showing a significant difference*
283 *showed prediction advantages for latent FC. C) Task activation prediction accuracies by condition. Pearson's*
284 *correlation was used to quantify the similarity of predicted-to-actual task activations using activity flow models with*
285 *connectivity based on either rest FC (red) or latent FC (blue). Error bars show the standard error of the mean*
286 *correlation. Asterisks indicate significant differences in similarity of beta activations from models based on latent FC*
287 *versus rest FC.*

288

289 **Latent FC improves prediction of general intelligence**

290 Our hypothesis that latent FC generalizes better than resting-state FC also predicts that
291 latent FC should be more related to general cognition and behavior, even behavior independent of
292 the particular tasks used for estimating the task-state FC going into the latent FC estimates. We
293 tested whether latent FC improves prediction of general intelligence using psychometric g to
294 capture many different behavioral and cognitive measures (Dubois, Galdi, Paul, & Adolphs, 2018;
295 Gottfredson, 1997). We estimated general intelligence (psychometric g) using a factor analysis
296 model on behavioral data from a range of cognitive tasks, then tested whether latent FC and/or rest
297 FC measures could predict general intelligence. We combined the exploration and validation
298 samples to increase the number of participants to 352 for this analysis, given the need for additional
299 participants (relative to the other analyses in this study) to achieve reasonable statistical power for
300 individual difference correlations (Yarkoni, 2009). We then employed a multiple linear regression
301 with ridge regularization approach to predict general intelligence from FC. However, one potential
302 confounding issue with simply pooling the full sample data is that the estimated factor scores for
303 latent FC and psychometric- g would be influenced by the data of to-be-predicted individuals,
304 introducing circularity into these analyses. To avoid this, we implemented a between-sample cross-
305 validation approach. Here, we estimated factor models for latent FC and psychometric- g scores in
306 each subsample separately (i.e., exploratory and validation), and predictions for the exploratory
307 subjects were generated from the validation sample regression model and vice versa.

308 We found that predicted general intelligence was significantly correlated with actual
309 general intelligence for models using both rest FC ($r = 0.26, p = 5.46e-07$) and latent FC ($r = 0.35,$
310 $p = 1.37e-11$) (Figure 5A). Consistent with our hypothesis, the model using latent FC significantly
311 improved prediction of general intelligence compared to the model using rest FC ($\Delta r = 0.09, t =$
312 $1.77, p = 0.04$, see Eid et al., 2011 for correlation comparison method). The magnitude of this
313 effect was large, as the percent linear variance explained by latent FC ($R^2 = 0.123$) was
314 approximately two times the percent linear variance explained by rest FC ($R^2 = 0.067$). In
315 comparison with the overall sample results, the correlation and difference in R^2 was larger for the
316 exploratory sample (Figure 5B) while the validation set showed a more-similar difference in R^2
317 despite lower correlations between predicted and actual psychometric g scores for both latent and
318 rest FC data (Figure 5C). A meta-analysis (Field, 2001) of the exploratory and validation samples
319 suggested that the pooled correlation difference effect was significant ($\Delta Z_{\text{pooled}} = 0.09, p = 0.016$)
320



321

322 **Figure 5. Relationship between actual and predicted general intelligence.** Results of ridge regression models from
323 rest FC and latent FC in the A) overall, B) exploratory, and C) validation sample. The significance of the difference
324 in correlation (Δr) is indicated below each plot. A meta-analysis of the exploratory and validation samples showed a
325 significant difference in the correlations between actual and predicted g scores when comparing rest to latent FC (Δz
326 = 0.09, $p = 0.016$).

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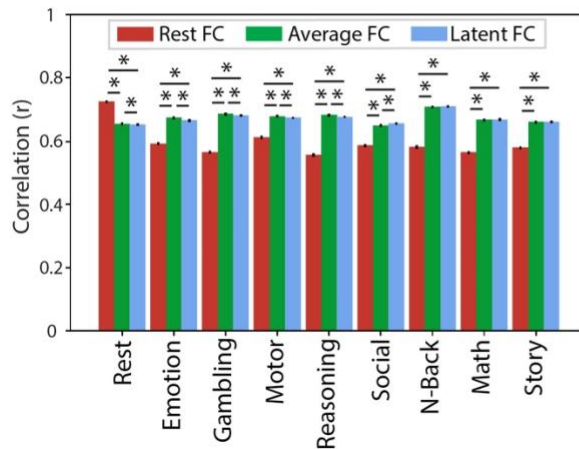
328 Comparing latent and average FC

329 While the factor model uses the covariance among the different states to compute optimal
330 weights, a simpler approach to finding consensus among states involves taking a simple average
331 across states. This approach assumes the weights/loadings between measured states are equal.

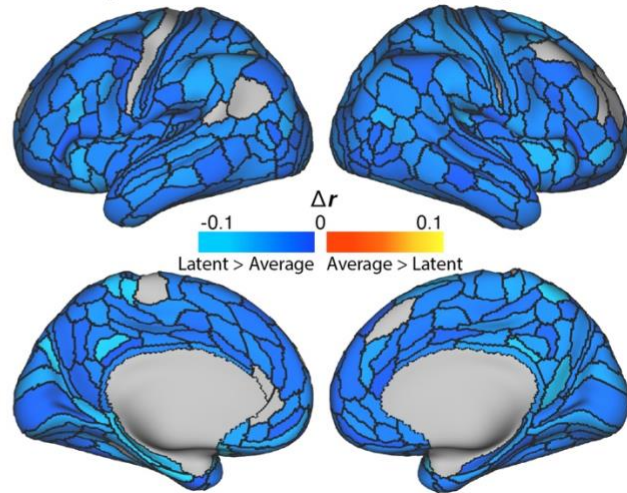
332 Given that the computed weights in our results with latent FC were relatively uniform across states,
333 we determined that this assumption was reasonable in this case. This supports the use of average
334 FC, however we directly compared latent FC to average FC to assess whether there were any
335 advantages to either method. To compare the factor model with a simple average, we computed
336 the mean value of each edge across states to construct an average connectivity matrix. For all
337 analyses, we controlled for the amount of data between rest and task. Results indicated that
338 combining across states, regardless of the approach, shows substantial improvements over using
339 even the full resting state data. Indeed, the average FC approach appears to out-perform the latent
340 FC approach (albeit only slightly) in generalizing to held-out connectivity states (Figure 6A). In
341 the activity flow mapping results, however, latent FC consistently outperforms average FC in
342 predicting regional activity patterns, showing better predictions in 348 out of 360 regions (97%),
343 whereas average FC showed no improved predictions (Figure 6B). Similarly, latent FC
344 outperformed average FC in condition-wise activity flow predictions in 22 out of 24 conditions
345 (Figure 6C). Together these results suggest that the average FC approach (sometimes termed
346 “general functional connectivity”) is a reasonable alternative to the more complex latent FC
347 approach, so long as the optimal weights across states are close to equal (an assumption not made
348 by latent FC). This difference between the methods would likely become more meaningful in cases
349 wherein a particular brain state is highly distinct from all others (e.g., deep sleep vs. conscious
350 states) or when one or more states is much noisier than the others (which would be weighted lower
351 by latent FC but not average FC).

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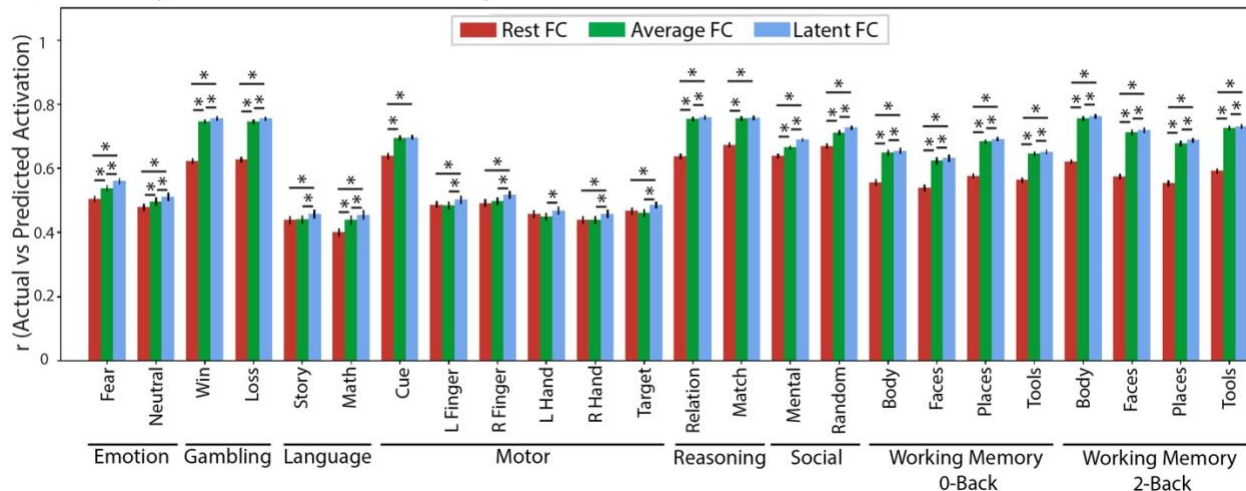
A) Generalizing Connectivity



B) Activity Flow Predictions: by region



C) Activity Flow Predictions: by condition



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Figure 6. Comparison of A) Generalizing connectivity and B) Activity flow models by region and C) condition, based on latent FC and average FC versus Rest. **A)** Both average (green) and latent (blue) FC outperformed rest FC on generalizing to all task states except resting state. Average FC performed similarly or slightly better than latent FC on all held-out states (asterisks denote significant differences, the higher position represents the test of rest vs latent FC). **B)** In contrast, latent FC outperformed average FC in predicting task activation in 97% of regions, whereas average FC outperformed in 0% regions. **C)** Across all conditions, latent FC was a better predictor than average FC of held-out activations (lower asterisks indicate significant difference between adjacent bars; higher asterisks indicate significant difference between latent and rest FC). All results control for the number of time points in the resting state data. For the validation sample results, see Figure S4.

364

Discussion

365

Defining a map of task-independent, intrinsic functional connections in the brain is a major

366

aim of basic research in cognitive neuroscience. Intrinsic FC persists across task states, making it

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a more reliable and generalizable measure of the underlying functional dynamics that shape

368 cognition and behavior. As such, measures of intrinsic FC are better candidates to serve as stable
369 biomarkers of important individual differences in behavioral outcomes (Elliott et al., 2019). We
370 utilized a factor analytic approach, a well-developed technique from measurement psychometrics
371 (Bollen, 2002), to define intrinsic FC as a latent variable derived from the common variances in
372 FC across task states. We compared the factor model against the standard approach applied in the
373 field, FC derived from resting state. The factor model not only shows enhanced measurement and
374 predictive properties beyond measures of intrinsic FC derived from resting state, it also offers a
375 unique theoretical perspective on the relationship between intrinsic and task-specific brain states.
376 In a latent variable model, individual task states are viewed as observable sample realizations of
377 the underlying intrinsic connectivity, and task-specific deviations from this baseline are modeled
378 as unique errors arising from a combination of noise and state-specific properties. The factor
379 modeling approach allows researchers to not only gain traction in defining intrinsic FC common
380 among brain states, but also to separate and explore properties that are specific to individuals and
381 states.

382 **Factor Analytic Model of Functional Connectivity**

383 We began by building factor analysis models of latent FC using two approaches. In the
384 first, we modeled latent FC using all available data. In this model, resting state functional
385 connections had the highest number of significant loadings of any condition. However, when
386 controlling for the number of time-points (by reducing the number of resting state timepoints to
387 match the tasks with shorter durations), resting state connections had the lowest percentage of
388 significant factor loadings. This property of the factor model highlights one of its strengths; higher
389 precision measurements show higher fidelity to the underlying common latent factor than lower-
390 precision measures. Here, the precision appears to be driven primarily by the amount of data.

391 However, in the absence of stringent data quality control, the factor model can also down-weight
392 poor-quality data (e.g., high motion, artifacts) relative to higher-quality data when variability
393 associated with noise does not replicate across task states.

394 Conversely, tasks that more closely represent underlying intrinsic FC will show stronger
395 factor loadings, similar to how the Raven's Progressive Matrices task loads highly onto the
396 generalized intelligence factor (Dubois et al., 2018). Given its widespread use as a marker of
397 intrinsic FC, we might have expected that resting state would load highly onto the latent FC factor
398 regardless of how much data went into its estimation. However, when controlling for the amount
399 of data used to estimate FC, the resting state loadings were lower than all other examined states,
400 even though there were still many more TRs of resting state than any one task state. Additionally,
401 when using the full amount of data to estimate rest FC, the factor loadings for resting state was
402 similar to the story and math tasks, each of which were estimated with much less data (Figure 2;
403 values in parentheses). These results suggest that resting state is not an especially good proxy for
404 intrinsic FC, which aligns with its relatively poor performance compared with latent FC in
405 predicting the patterns of connectivity and evoked brain activity observed for other states.

406 **Latent FC as a Reliable Measure of Intrinsic Connectivity**

407 As mentioned previously, a marker of intrinsic connectivity is its persistence across task
408 states (i.e., generalizability), as well as its ability to accurately recapitulate observed realizations
409 of evoked brain activity and connectivity (Elliott et al., 2019, 2020; Kragel, Han, Kraynak,
410 Gianaros, & Wager, 2020; Parkes, Satterthwaite, & Bassett, 2020). Our results highlight the
411 advantages of latent versus rest FC to reliably predict independent connectivity and regional
412 activations. When comparing patterns of connectivity, we showed that latent FC showed higher
413 correlation with held-out, task-specific connectivity states compared with rest FC, with the sole

414 exception of resting state connectivity where rest FC outperformed. This pattern of results suggests
415 that resting state FC is less generalizable as a measure of intrinsic connectivity and instead there
416 are resting state-specific factors which shape the dynamics of rest FC that are not present in other
417 states.

418 One potential explanation for this might be that tasks as a group reliably differ from rest FC's more
419 intrinsic profile, and the reduction in generalizability reflects deviations from a default state. Under
420 this explanation, the latent FC advantage could simply reflect that there are more task indicators
421 in the measurement model than rest (although note that even when controlling for number of
422 timepoints, the amount of rest data is equal to all the tasks combined) and we would predict that
423 latent FC would be a poorer representation of rest FC patterns of connectivity. However, results
424 did not show a substantial drop in the correlation of latent and rest FC compared to the correlations
425 of latent FC with the various task FC patterns (blue bars, Figure 3). Indeed, it is when we used rest
426 FC as the predictor that we observed reductions in its correlation with task connectivity, compared
427 with resting state (red bars, Figure 3). This suggests that latent FC does a better job of representing
428 common, stable variability in FC profiles across both resting and task states. Importantly, latent
429 FC does so even though the task or rest condition being correlated is left out of the factor model
430 for that specific comparison to avoid circularity. As such, the factor score analytically has different
431 indicators across all comparisons, and nevertheless still outperforms rest FC. Moreover, obtaining
432 a better sample of the resting state by using the full time series resulted in the resting state having
433 the highest factor loadings and a strongest correlation with latent FC, which suggests that over
434 time the resting state converges to latent FC.

435

436 The advantages of latent FC are not, however, restricted to the connectivity space; the latent
437 measure of intrinsic FC also outperforms rest FC in predicting state-specific activation patterns.
438 Not only did latent FC support higher prediction accuracy by the activity flow model of task
439 activation globally ($r_{latent} = 0.66$ vs. $r_{rest} = 0.56$), it showed condition-specific advantages in 23 out
440 of 24 specific task conditions (Figure 4B). Rest FC, in comparison, displayed higher prediction
441 accuracy in none of the task conditions (in the left-hand motor condition, latent and rest FC
442 performed comparably; Figure 4C). When we examined predictions of region-specific patterns of
443 activation, results showed that latent FC had improved prediction over rest FC for 68% of all brain
444 regions across a variety of distributed networks. In contrast, rest FC showed improved prediction
445 for only 1.1% of regions, all of which were restricted to the VIS2 network (and constituted only
446 7% of that network). These improvements, as before, were not due to circularity in the analyses,
447 as task predictions using latent FC were done using the leave-one-task-out approach in the factor
448 model.

449 **Improving External Validity with Latent FC**

450 While latent FC has demonstrable advantages for prediction within the brain, its utility as
451 a method of estimating brain-based biomarkers relies on its predictive validity for outcomes of
452 interest. Here, we showed that connectivity values from latent FC showed superior prediction of a
453 metric of generalized intelligence (psychometric g) than did rest FC connections. Although both
454 rest FC and latent FC values significantly predicted individual differences in generalized
455 intelligence, latent FC nearly doubled the percent of explained variance in the outcome over rest
456 FC (~12% versus ~7%). In measurement science, this is a hallmark advantage of the latent variable
457 approach used in factor analysis. Methods which fail to account for measurement error tend to
458 show reduced relationships between variables, whereas modeling state-specific error terms dis-

459 attenuates those relationships (Schmidt & Hunter, 1996). Indeed, generalized intelligence is
460 generally modeled with a factor analytic approach for precisely this reason. We demonstrate that
461 the framework for improving measurement properties in behavioral measures applies equally to
462 measures derived from functional neuroimaging data. As such, factor analytic models are ideal for
463 aiding the search for biomarkers across a wide domain of individual difference outcomes.
464 Furthermore, more reliable estimates of FC may aid modeling efforts that use intermediate network
465 metrics (e.g., modularity, hub diversity) to predict participant behavior (e.g., (Bertolero, Yeo,
466 Bassett, & D’Esposito, 2018)), offer an exciting range of possible uses for latent FC in future work.

467 **State Aggregation Improves Predictive Performance**

468 The performance of average FC suggests that aggregating information across states has
469 advantages over longer scan sessions of resting state, regardless of the approach used.
470 Interestingly, average FC performance is not uniform in relation to the latent FC, performing as-
471 good or slightly better than latent FC in correlating with state-specific connectivity, but
472 underperforming latent FC in predicting held out activity in almost all regions. A few
473 circumstances may predict when we would expect to see more or less pronounced differences
474 between average and latent FC. First, data quality: We expect more pronounced differences for
475 lower quality data and less pronounced differences for higher quality data. The HCP data used
476 here is of extremely high quality, which reduces variability in noise between scans. This is
477 reflected in the average factor loadings which are relatively close in value across states (Figure 2).
478 Of course, as the loadings converge in value, the more similar average and latent FC will become
479 (here the connectivity values are correlated; $r = .98$). Second, the method of factor analysis used:
480 Here, we opted to fit a single-factor model for each connection independently due to the large
481 number of operations (e.g., separate models for each connection). However, a single factor in

482 isolation may not be the best fit for brain data (van Kesteren & Kievit, 2020) and the method here
483 might represent a sort of floor performance for latent FC relative to approaches which adopt a
484 dependent model that tries to optimize the fit for each factor model.

485 Finally, there appear to be differences depending on the type of dependent variable in
486 question. For example, while the factor and average models converge in their correlation with
487 connectivity for held-out states, we found that activity flow models that incorporated latent FC
488 performed better. Average and factor models produced similar patterns of relative connectivity
489 (i.e., highly correlated patterns of FC), however the distribution of connectivity values differ.
490 Latent FC estimates exhibited a sparser distribution of connectivity by zero-ing out low and/or
491 unstable connections, which may have improved the activity flow models by reducing the
492 contributions of disconnected brain regions (see Figure S5).

493 Despite the relatively small differences in performance between average and latent FC,
494 there are theoretical reasons to prefer a latent variable perspective for FC estimation. The first, as
495 mentioned before, is that while the average FC must assume equal loadings, latent FC makes this
496 a testable hypothesis. If loadings converge towards equal values, then average and latent FC will
497 converge (as they nearly did here). This suggests that averaging will likely perform well under
498 conditions similar to the HCP data (high quality, young adult data). However, as the data diverges
499 from this baseline, latent FC should have advantages by weighting data according to how closely
500 it reflects intrinsic functional states and contributes to the common variance across measures. If
501 differences among measures increase (i.e., measures reflect intrinsic FC better or worse), we would
502 hypothesize that average and latent FC would diverge in their performance. We can see this in a
503 small reproducible example (see Supplemental Code Demonstrations), where more variable
504 loadings impact the ability of sums scores, but not factor scores, to predict a hypothetical outcome

505 variable. However, apart from these practical considerations, a latent variable model of FC is a
506 good theoretical model for how state-specific functional connections emerge from underlying,
507 intrinsic neural connectivity. Intrinsic connectivity is an unobserved state (Bollen, 2002) that gives
508 rise to state specific phenotypes based on combinations of common (i.e., the latent factor) and
509 state-specific (i.e., the error) variance.

510 **Conclusions**

511 In summary, we utilized a factor analytic approach to derive intrinsic FC from multiple
512 task and resting state data. Our derived measure, termed latent FC, showed improved
513 generalizability and reliability compared to a standard measure of resting-state FC. Not only did
514 latent FC do a better job of reflecting state-specific FC patterns across tasks, it also
515 overwhelmingly improved predictions of regional activations when utilized in activity flow
516 models. Finally, connectivity derived from latent FC doubled the predictive utility of an external
517 measure of generalized intelligence (*g*) compared with connectivity from rest FC, highlighting its
518 suitability for use in clinical and other individual difference research, where reliable biomarkers
519 are needed. These results present compelling support for the use of factor analytic models in
520 cognitive neuroscience, demonstrating the value of established tools from psychometrics for
521 enhancing measurement quality in neuroscience.

522

523

Materials and Methods

524 For clarity, portions of the text in this section are from our prior publication using the same
525 dataset and some identical analysis procedures: Ito et al. (2020).

526

Participants

527 Data in the present study were collected as part of the Washington University-Minnesota
528 Consortium of the Human Connectome Project (HCP) (Van Essen et al., 2013). A subset of data (
529 $n = 352$) from the HCP 1200 release was used for empirical analyses. Specific details and
530 procedures of subject recruitment can be found in Van Essen et al. (2020). The subset of 352
531 participants was selected based on: quality control assessments (i.e., any participants with any
532 quality control flags were excluded, including 1) focal anatomical anomaly found in T1w and/or
533 T2w scans, 2) focal segmentation or surface errors, as output from the HCP structural pipeline, 3)
534 data collected during periods of known problems with the head coil, 4) data in which some of the
535 FIX-ICA components were manually reclassified; exclusion of high-motion participants
536 (participants that had any fMRI run in which more than 50% of TRs had greater than 0.25mm
537 framewise displacement); removal according to family relations (unrelated participants were
538 selected only, and those with no genotype testing were excluded). A full list of the 352 participants
539 used in this study will be included as part of the code release.

540 All participants were recruited from Washington University in St. Louis and the
541 surrounding area. We split the 352 subjects into two cohorts of 176 subjects: an exploratory cohort
542 (99 women) and a validation cohort (84 women). The exploratory cohort had a mean age of 29
543 years of age (range=22-36 years of age), and the validation cohort had a mean age of 28 years of
544 age (range=22-36 years of age). All subjects gave signed, informed consent in accordance with the
545 protocol approved by the Washington University institutional review board.

546 **Scan Acquisition**

547 Whole-brain multiband echo-planar imaging acquisitions were collected on a 32-channel
548 head coil on a modified 3T Siemens Skyra with TR=720 ms, TE=33.1 ms, flip angle=52°,
549 Bandwidth=2,290 Hz/Px, in-plane FOV=208x180 mm, 72 slices, 2.0 mm isotropic voxels, with a

550 multiband acceleration factor of 8. Data for each subject were collected over the span of two days.
551 On the first day, anatomical scans were collected (including T1-weighted and T2-weighted images
552 acquired at 0.7 mm isotropic voxels) followed by two resting-state fMRI scans (each lasting 14.4
553 minutes) and ending with a task fMRI component. The second day consisted of first collecting a
554 diffusion imaging scan, followed by a second set of two resting-state fMRI scans (each lasting
555 14.4 minutes), and again ending with a task fMRI session.

556 Each of the seven tasks was collected over two consecutive fMRI runs. The seven tasks
557 consisted of an emotion cognition task, a gambling reward task, a language task, a motor task, a
558 relational reasoning task, a social cognition task, and a working memory task. Briefly, the emotion
559 cognition task required making valence judgements on negative (fearful and angry) and neutral
560 faces. The gambling reward task consisted of a card guessing game, where subjects were asked to
561 guess the number on the card to win or lose money. The language processing task consisted of
562 interleaving two language conditions, which involved answering questions related to a story
563 presented aurally, and a math condition, which involved basic arithmetic questions presented
564 aurally. Note that we treated the two language task conditions as separate tasks, given the highly
565 distinct nature of the conditions (other than that they were presented aurally). The motor task
566 involved asking subjects to either tap their left/right fingers, squeeze their left/right toes, or move
567 their tongue. The reasoning task involved asking subjects to determine whether two sets of objects
568 differed from each other in the same dimension (e.g., shape or texture). The social cognition task
569 was a theory of mind task, where objects (squares, circles, triangles) interacted with each other in
570 a video clip, and subjects were subsequently asked whether the objects interacted in a social
571 manner. Lastly, the working memory task was a variant of the N-back task. Further details on the

572 resting-state fMRI portion can be found in (Smith et al., 2013), and additional details on the task
573 fMRI components can be found in (Barch et al., 2013) .

574 **Behavior: Data**

575 To assess generalized intelligence (g), we drew 11 measures of cognitive ability from the
576 HCP dataset, which are derived from the NIH Toolbox for Assessment of Neurological and
577 Behavioral function (<http://www.nihtoolbox.org>; (Gershon et al., 2013) and the Penn
578 computerized neurocognitive battery (Gur et al., 2010). Tasks included: picture sequence memory;
579 dimensional card sort; flanker attention and inhibitory control; the Penn Progressive Matrices; oral
580 reading recognition; picture vocabulary; pattern completion processing speed; variable short Penn
581 line orientation test; Penn word memory test (number correct and median reaction time as separate
582 variables]) and list sorting. For all measures, the age-unadjusted score was used where applicable.
583 For complete information regarding all measures, see the descriptions in the Cognition Category
584 of the HCP Data Dictionary
585 ([https://wiki.humanconnectome.org/display/PublicData/HCP+Data+Dictionary+Public-
586 +Updated+for+the+1200+Subject+Release](https://wiki.humanconnectome.org/display/PublicData/HCP+Data+Dictionary+Public-+Updated+for+the+1200+Subject+Release)).

587 **Behavior: Factor analysis model of psychometric ‘g’**

588 We then derived a general factor of intelligences using a multiple-indicator latent factor
589 model. We approach the factor model using a confirmatory factor analysis (CFA) approach with a
590 unitary factor underlying all individual cognitive tasks. Factor loadings were estimated using the
591 *psych* R package (Revelle, 2017). Factor scores were computed using the regression method
592 (Thurstone, 1935) to obtain manifest variables for prediction.

593 **fMRI: Preprocessing**

594 Minimally preprocessed data for both resting-state and task fMRI were obtained from the
595 publicly available HCP data. Minimally preprocessed surface data was then parcellated into 360
596 brain regions using the Glasser atlas (Glasser et al., 2016). We performed additional preprocessing
597 steps on the parcellated data for resting-state fMRI and task state fMRI to conduct neural
598 variability and FC analyses. This included removing the first five frames of each run, de-meaning
599 and de-trending the time series, and performing nuisance regression on the minimally preprocessed
600 data (Ciric et al., 2017) . Nuisance regression removed motion parameters and physiological noise.
601 Specifically, six primary motion parameters were removed, along with their derivatives, and the
602 quadratics of all regressors (24 motion regressors in total). Physiological noise was modeled using
603 aCompCor on time series extracted from the white matter and ventricles (Behzadi, Restom, Liau,
604 & Liu, 2007) . For aCompCor, the first 5 principal components from the white matter and
605 ventricles were extracted separately and included in the nuisance regression. In addition, we
606 included the derivatives of each of those components, and the quadratics of all physiological noise
607 regressors (40 physiological noise regressors in total). The nuisance regression model contained a
608 total of 64 nuisance parameters. This was a variant of previously benchmarked nuisance regression
609 models reported in (Ciric et al., 2017) .

610 We excluded global signal regression (GSR), given that GSR can artificially induce
611 negative correlations (Murphy, Birn, Handwerker, Jones, & Bandettini, 2009; Power et al., 2014),
612 which could bias analyses of whether global correlations decrease during task performance. We
613 included aCompCor as a preprocessing step here given that aCompCor does not include the
614 circularity of GSR (regressing out some global gray matter signal of interest) while including some
615 of the benefits of GSR (some extracted components are highly similar to the global signal) (Power
616 et al., 2018). This logic is similar to a recently-developed temporal-ICA-based artifact removal

617 procedure that seeks to remove global artifact without removing global neural signals, which
618 contains behaviorally relevant information such as vigilance (Glasser et al., 2018; Wong, Olafsson,
619 Tal, & Liu, 2013). We extended aCompCor to include the derivatives and quadratics of each of
620 the component time series to further reduce artifacts. Code to perform this regression is publicly
621 available online using python code (version 2.7.15) ([https://github.com/ito-](https://github.com/ito-takuya/fmriNuisanceRegression)
622 [takuya/fmriNuisanceRegression](https://github.com/ito-takuya/fmriNuisanceRegression)). Following nuisance regression, the time series for each run
623 (task-state and rest-state) were z-normalized such that variances across runs would be on the same
624 scale (i.e., unit variance).

625 Task data for task FC analyses were additionally preprocessed using a standard general
626 linear model (GLM) for fMRI analysis. For each task paradigm, we removed the mean evoked
627 task-related activity for each task condition by fitting the task timing (block design) for each
628 condition using a finite impulse response (FIR) model (Cole et al., 2019) . (There were 24 task
629 conditions across seven cognitive tasks.) We used an FIR model instead of a canonical
630 hemodynamic response function given recent evidence suggesting that the FIR model reduces both
631 false positives and false negatives in the identification of FC estimates (Cole et al., 2019). This is
632 due to the FIR model's ability to flexibly fit the mean-evoked response across all blocks.

633 FIR modeled task blocks were modeled separately for task conditions within each of the
634 seven tasks. In particular, two conditions were fit for the emotion cognition task, where coefficients
635 were fit to either the face condition or shape condition. For the gambling reward task, one condition
636 was fit to trials with the punishment condition, and the other condition was fit to trials with the
637 reward condition. For the language task, one condition was fit for the story condition, and the other
638 condition was fit to the math condition. For the motor task, six conditions were fit: (1) cue; (2)
639 right hand trials; (3) left hand trials; (4) right foot trials; (5) left foot trials; (6) tongue trials. For

640 the relational reasoning task, one condition was fit to trials when the sets of objects were matched,
641 and the other condition was fit to trials when the objects were not matched. For the social cognition
642 task, one condition was fit if the objects were interacting socially (theory of mind), and the other
643 condition was fit to trials where objects were moving randomly. Lastly, for the working memory
644 task, 8 conditions were fit: (1) 2-back body trials; (2) 2-back face trials; (3) 2-back tool trials; (4)
645 2-back place trials; (5) 0-back body trials; (6) 0-back face trials; (7) 0-back tool trials; (8) 0-back
646 place trials. Since all tasks were block designs, each time point for each block was modeled
647 separately for each task condition (i.e., FIR model), with a lag extending up to 25 TRs after task
648 block offset.

649 **fMRI: Task activation**

650 We performed a standard task GLM analysis on fMRI task data to estimate evoked brain
651 activity during task states. The task timing for each of the 24 task conditions was convolved with
652 the SPM canonical hemodynamic response function to obtain task-evoked activity estimates
653 (Friston et al., 1994). Coefficients were obtained for each parcel in the Glasser et al. (2016) cortical
654 atlas for each of the 24 task conditions.

655 **fMRI: Functional connectivity (FC) estimation**

656 Residual timeseries from the rest and task nuisance regressions were used to estimate
657 functional connectivity for each task. Connectivity values were estimated using zero-lag Pearson
658 product-moment correlations. Timeseries were concatenated across separate runs of the same task
659 to yield a single connectivity value per edge for a given task or resting state condition. For each
660 task scan, we utilized TRs that corresponded to “on-task” timepoints. For instance, we extracted
661 TRs from the working memory scan during N-back task blocks, excluding TRs from the inter-

662 block fixation periods. For the number of TRs included in the connectivity estimates for each
663 condition and scan state, see Table S1.

664 **fMRI: Factor analysis model of latent FC**

665 Factor analysis for obtaining latent FC was conducted with the same approach used to
666 obtain factor scores for generalized intelligence. FC estimates from each separate fMRI task were
667 used as indicators on a unitary factor model and factor scores were obtained using the regression
668 method in the *psych* R package. A separate model was computed for each edge in the connectivity
669 adjacency matrix. We took several approaches to test the predictive utility of latent FC for
670 activation and behavior (detailed below).

671 The first set of analyses tested two alternative measurement approaches for latent FC. The
672 first was to utilize all available data from each functional scan to estimate factor scores for each
673 edge. However, because of the differential amount of scan time for different functional runs (e.g.,
674 ~58 minutes of resting-state versus ~10 minutes of working memory scans), we might expect
675 indicators (i.e., scan types) with more data would dominate the measurement model in the factor
676 analysis. To control for this potential confound, we ran additional analyses where indicators were
677 constrained to have equivalent numbers of TRs used to estimate individual scan functional edges
678 between task and rest, and between different task states. The reasoning task had the fewest “on-
679 task” TRs (264) and therefore served as the limiting factor for task scans data. As such, 264 TRs
680 of each task (for 2112 TRs of task) and a corresponding 2112 TRs of rest were used in these
681 analyses. All of these analyses were performed modeling all available scan types in the same factor
682 model.

683 For activity flow mapping (ActFlow) analyses (Cole et al., 2016; Ito et al., 2020), where
684 activations in held-out regions were predicted using estimated activity flowing over estimated

685 connections, latent FC was estimated independently for each connection by applying leave-one-
686 state-out factor analysis (LOSO-FA) on the state FC estimates to prevent circularity in the
687 predictive model. For instance, when predicting activation in the emotion task, FC estimates were
688 obtained without including the emotion task as an indicator in the factor model. In all ActFlow
689 analyses, we estimated predictions per subject and then pooled results (i.e., an estimate-then-
690 average approach).

691 **Meta-Analysis Across Samples**

692 To appropriately combine effects of the g -prediction analysis across the validation and
693 exploratory sample, we computed r -to- z -score transformations of the individual coefficients and
694 then combined them into a weighted z score using the standard formula (Field, 2001) where z is
695 the z -score and the weight (w) corresponds to the sample size.

696
$$\bar{z}_r = \frac{\sum_i^k w_i z_{ri}}{\sum_i^k w_i}$$

697

698 The significance of this meta-analytic parameter was determined using a chi-square test (Field,
699 2001).

700

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712

713 **Author contributions**

714 KLA and MWC designed the analytic approach. EMM and KLA carried out analyses with
715 MWC. EMM, KLA, and MWC wrote the manuscript, with feedback received from all other
716 authors.

717

718 **Conflict of interest**

719 The authors declare no competing financial interests.

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