

1 **Similarity in sensory modality and information domain impair**
2 **processing in a dual-task context: Evidence from behavior,**
3 **pupillometry, and EEG**

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24 **Project Abstract**

25 Perception and navigation frequently require us to maintain sensory information in memory, while
26 also processing new sensory inputs as they arise. Recent fMRI research has uncovered regions in
27 human frontal cortex that coordinate these diverse processes. Across various attention and working
28 memory (WM) tasks, these regions can be separated into two distinct networks. Each shows a
29 response preference for either auditory or visual stimuli, yet in addition, each can be flexibly
30 recruited based on the information domain (i.e., temporal or spatial) of the task, regardless of
31 sensory modality. Motivated by the sensory and functional specializations these networks display,
32 we investigated whether dual-task interference is affected by similarity between the tasks in
33 sensory modality (auditory or visual) and information domain. Participants performed a novel
34 dual-task paradigm involving different combinations of WM and Intervening tasks, while two
35 temporally sensitive physiological signals, pupillometry and electroencephalography (EEG), were
36 measured. Convergent evidence from behavioral performance, pupil dilation amplitudes, and
37 event-related potentials (ERPs) indicates that dual-task interference is greatest when the tasks
38 match in both sensory modality and information domain. However, differences also arise in the
39 patterns of dual-task interference across these metrics, highlighting the differential strengths and
40 sensitivities of each. The results are consistent with increased interference when multiple tasks
41 compete for shared cognitive control resources due to a common sensory modality or information
42 domain.

43

44 **Keywords:** Dual-task, audio-visual, working memory, attention, pupillometry, EEG, alpha,
45 lateral frontal cortex (LFC)

46

47 **Introduction**

48 Perceiving and acting in real-world environments requires a massive coordination of neural
49 processes. We must extract spatial and temporal information about objects in our environment
50 from multiple sensory modalities – particularly vision and audition – and store this information in
51 working memory (WM) to guide future actions. Meanwhile, our perceptual systems must be
52 flexible enough to process salient new sensory inputs as they arise without disrupting the
53 information stored in WM. Recent fMRI research has identified sensory-biased networks in the
54 human lateral frontal cortex (LFC) that may coordinate this interplay between sensory processing
55 and WM. The LFC had previously been implicated in a wide array of cognitive functions,
56 including working memory, sensorimotor control, and language processing, leading it to be
57 frequently labelled a “multiple demand” structure (Assem et al., 2020; Blank et al., 2014; Duncan
58 & Owen, 2000; Fedorenko et al., 2013; Postle et al., 2000). However, at the individual-participant
59 level, distinct subregions within the LFC can be reliably identified with a preference for auditory
60 or visual processing during attention and WM tasks (Braga et al., 2017; Mayer et al., 2016;
61 Michalka et al., 2015; Noyce et al., 2017). Intrinsic functional connectivity analyses have revealed
62 that these subregions are preferentially connected to the corresponding sensory brain areas,
63 forming networks tuned to processing either auditory or visual information and storing it in WM
64 (Michalka et al., 2015; Tobyne et al., 2017).

65 Importantly, processing in these LFC subregions is not strictly confined to information in
66 the preferred sensory modality. Rather, the complementary LFC network can also be recruited
67 depending on whether the information being processed is temporal or spatial in nature (Michalka
68 et al., 2015). Vision and audition have complementary specializations for spatial and temporal
69 processing, respectively. From the retina, visual representations are inherently spatial, and neural

70 maps of space are found throughout the visual processing pathway (Silver & Kastner, 2009;
71 Stensaas et al., 1974; Swisher et al., 2007). At various stages along this pathway, visual neurons
72 are sensitive to particular spatial features, such as edges, object orientation, spatial frequency, and
73 texture (Hubel & Wiesel, 1959; Issa et al., 2000). Auditory spatial information, on the other hand,
74 must be indirectly computed based on interaural cues. The peripheral auditory system is instead
75 tuned to temporal information, with auditory nerve fibers capable of phase-locking to oscillating
76 sound pressure waves (Dynes & Delgutte, 1992). This temporal sensitivity allows the auditory
77 system to be organized around sound frequency (Da Costa et al., 2011; Merzenich & Brugge, 1973;
78 Wessinger et al., 1997), and for perceptual judgement of inter-stimulus intervals to be much more
79 precise in audition than vision (Lhamon & Goldstone, 1974). Reflecting this temporal
80 specialization of the auditory system, the auditory-biased LFC network can be recruited by visual
81 inputs if the task requires temporal information processing. Similarly, the visual-biased LFC
82 network is recruited by auditory inputs if spatial information processing is required (Michalka et
83 al., 2015). This flexible allocation of resources allows information to be processed by a network
84 geared to the complementary strengths of each sensory modality.

85 Given what is known about recruitment in these sensory-biased cortical networks, in the
86 present study we tested the prediction that dual-task interference will depend on whether the two
87 tasks share the same sensory modality (auditory vs. visual) and information domain (temporal vs.
88 spatial), thus causing the tasks to rely upon processing within the same cortical network. We
89 developed a dual-task interference paradigm featuring WM and “Intervening” tasks. The WM task
90 required participants to remember temporal or spatial information about a set of auditory or visual
91 stimuli, while the Intervening task – presented during WM retention – required participants to
92 make an immediate perceptual judgment about either the timing or spatial locations of auditory

93 stimuli. This design was inspired by “multiple resource theory,” which posits that two tasks will
94 interfere with each other when they draw on the same pool of neural resources (Navon & Gopher,
95 1979; Nickerson, 1980; Wickens, 2002). This paradigm allowed us to observe patterns of
96 interference as participants engaged a WM network to encode sensory information in memory,
97 performed a real-time perceptual task that required either increasing the load on the active network
98 or switching networks, and finally retrieved the information stored in WM.

99 To gain insights about the temporal dynamics of dual task interference in this paradigm,
100 we combined behavioral measures with two temporally sensitive indexes of cognitive processing:
101 pupillometry and electroencephalography (EEG). Task-evoked pupil dilations dynamically reflect
102 task difficulty or the participant’s effort level during task performance (Causse et al., 2016;
103 Gilzenrat et al., 2012; Murphy et al., 2011; Winn et al., 2015). EEG signals reveal different stages
104 of processing through event-related potentials (ERPs) that are phase locked to sensory events
105 (Luck, 2012), and more loosely coupled changes in oscillatory power in stereotypical frequencies
106 that have been linked to different cognitive states (Ward, 2003). These techniques provide multiple
107 viewpoints into dual-task interference with high temporal precision, but importantly, they lack the
108 spatial resolution necessary to directly implicate the complementary sensory-biased cortical
109 networks. Nonetheless, the WM tasks in this study were derived from the tasks Michalka et al.
110 (2015) used to characterize the complementary LFC networks. Thus, we can say with relative
111 confidence that the specific temporal and spatial WM tasks used in the current paradigm
112 differentially engaged these networks.

113 In conditions with greater interference, we expected to observe the following phenomena:
114 increased behavioral errors, both in WM retrieval and auditory perceptual judgments in the
115 Intervening task; larger maximum pupil dilations; reduced ERP amplitudes, reflecting the strain

116 on neural resources needed to process the stimuli; and differing oscillatory signatures. In
117 considering neural oscillations, we were specifically interested in the theta (4-8 Hz) and alpha (8-
118 13 Hz) frequency bands, both of which have been implicated in task switching and WM
119 maintenance (Bastiaansen et al., 2002; Cunillera et al., 2012; López et al., 2019; Obleser et al.,
120 2012; Sauseng et al., 2006).

121 In brief, convergent evidence from behavior, pupillometry, and EEG indicated that
122 interference was generally elevated when the WM and Intervening tasks relied on the same
123 modality- and domain-biased attention and WM network. When the sensory modality differed
124 between tasks, behavioral and autonomic signatures of interference were weak and
125 indistinguishable based on WM domain. In these conditions, however, ERP amplitudes and alpha
126 oscillations uncovered subtler patterns of domain-based interference. These results indicate that
127 switching between complementary attention and WM networks comes at a lower cost than loading
128 processing onto a single network.

129

130

131 **Materials and Methods**

132 *Participants*

133 Twenty-three healthy young adults completed all experimental procedures. Data from three
134 participants was removed due to excessive noise in the pupillometry or EEG data, making for a
135 final sample of twenty individuals (13 female, mean age 20.9 years, standard deviation 2.3 years).
136 One additional participant was excluded from only the time-frequency analyses due to anomalous
137 high-frequency noise in their EEG data. All participants had normal or corrected-to-normal visual
138 acuity and no reported colorblindness. Participants who wore glasses for visual correction and

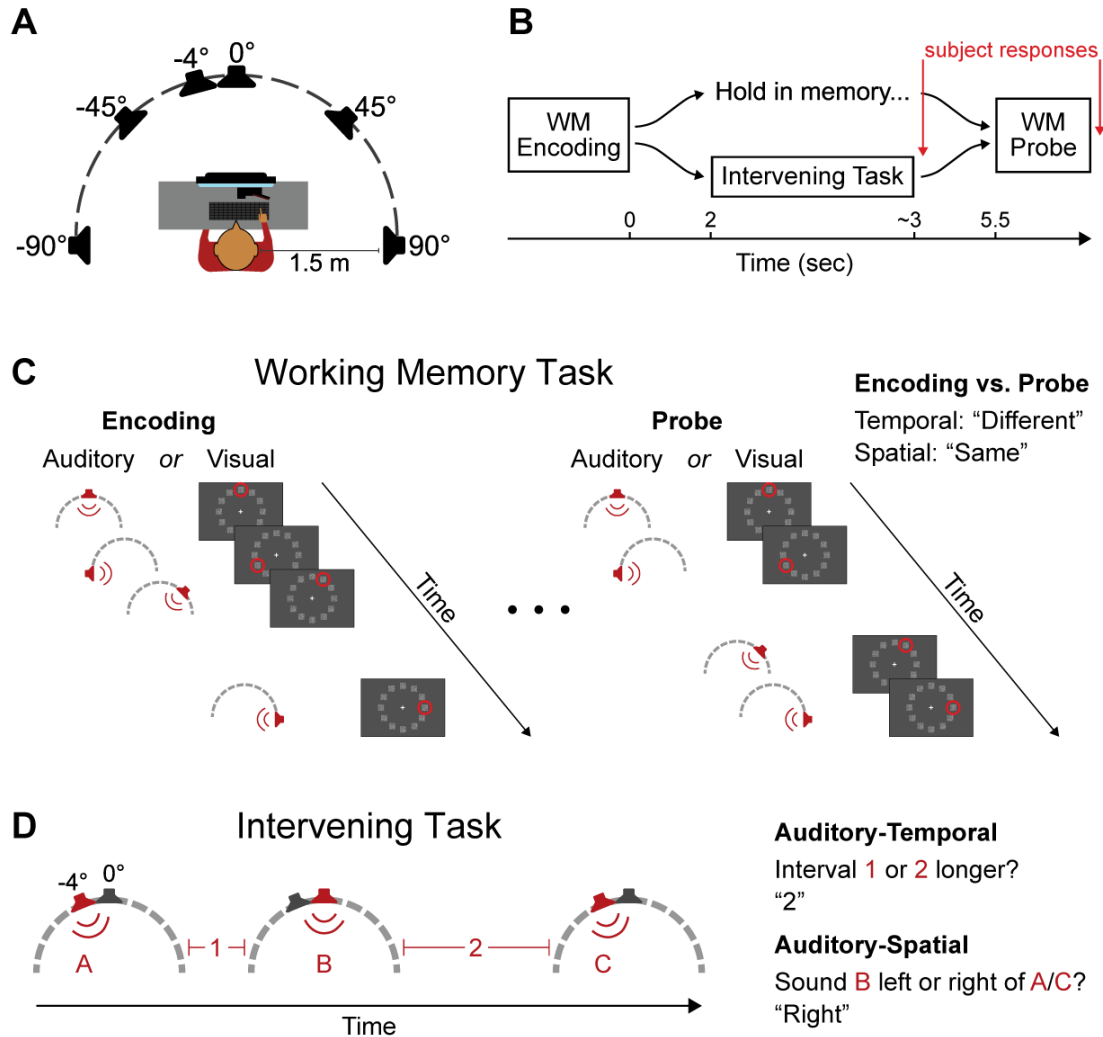
139 could not use contact lenses were excluded to avoid potential artifacts in the pupillometry data.
140 All participants had clinically normal hearing, defined by tone detection thresholds below 20 dB
141 HL at octave frequencies between 250 Hz and 8 kHz, as confirmed by an audiometric screening.
142 Participants gave written informed consent and were compensated for their participation. All study
143 procedures were approved by the Boston University Charles River Campus Institutional Review
144 Board.

145

146 *Experimental Setup*

147 The experiment was conducted in a darkened, electrically shielded, sound-treated booth.
148 Participants were seated comfortably with their chin resting on a desk-mounted head support (SR
149 Research). A Benq 1080p LED monitor (27-inch diagonal, 120 Hz refresh rate) was positioned in
150 front of the participant at approximately 65 cm distance. The monitor was set to 3% of its
151 maximum brightness level to prevent eye fatigue and pupil diameter saturation. An EyeLink 1000
152 Plus eye tracking system was placed on the desk just below the display for measurement of pupil
153 diameter. Six free-field loudspeakers (KEF E301) were mounted in an arc around the participant
154 at a distance of 1.5 m. Five of the loudspeakers were equally spaced in azimuth at $\pm 90^\circ$, $\pm 45^\circ$, and
155 0° relative to midline; the sixth was placed immediately to the left of the central loudspeaker, at
156 -4° azimuth, and used only in the Intervening tasks (Fig. 1A). All six loudspeakers were positioned
157 at approximately 5° elevation relative to the horizontal plane of the eyes to reduce obstruction by
158 the visual display. Auditory stimulus presentation was handled using an RME Fireface UCX
159 soundcard.

160



161

162 **Figure 1: Experimental setup and task design.** **A**, Overhead depiction of the experimental setup. All the
 163 loudspeakers except the one at -4° azimuth were used for the WM tasks, while only the loudspeakers at
 164 -4° and 0° were used for the Intervening tasks. **B**, Overall dual-task structure. The time base is relative to
 165 the offset of the final stimulus in the WM encoding phase. **C**, WM task structure. Loudspeakers playing
 166 each auditory stimulus and the changing visual stimuli are shown in red. Sensory modality always matched
 167 between the encoding and probe sequences. Correct responses for this example trial, shown on the right,
 168 differ depending on whether task was temporal or spatial. Note that in the actual experiment, inter-stimulus
 169 intervals were always isochronous in the auditory-spatial WM task. **D**, Intervening task structure. Auditory
 170 stimuli and inter-stimulus intervals are numbered and referred to in the temporal and spatial task responses
 171 on the right.

172

173 A standard keyboard was used to register all task responses. 64-channel EEG data was
 174 collected at a sampling rate of 2048 Hz using a Biosemi ActiveTwo system. Separate PCs were
 175 used for pupillometry recording and EEG recording, and a third PC was used for presenting stimuli

176 and registering behavioral responses. To ensure synchrony of event triggers (e.g. trial starts,
177 stimulus presentation) between the pupillometry and EEG data, triggers were output through the
178 S/PDIF channel on the soundcard, converted to TTL pulses using a custom converter box, and
179 written simultaneously into the EEG and pupillometry data files. Experiment control was carried
180 out using custom MATLAB software, and visual stimulus presentation was implemented using
181 the Psychtoolbox package (Brainard, 1997).

182

183 *Task and Experimental Design*

184 Participants performed a dual-task paradigm, comprising a working memory (WM) task
185 and an Intervening task (Fig. 1B). Each trial started with a 1.5-second baseline period, followed
186 by the presentation of a sequence of four auditory or visual stimuli to be encoded in WM. Each
187 stimulus was presented at one of five (auditory) or twelve (visual) locations, and each inter-
188 stimulus interval in the sequence was randomly set to be either short or long (more details below).
189 The WM task could be either temporal or spatial, yielding four total WM task conditions: auditory-
190 temporal (AT), auditory-spatial (AS), visual-temporal (VT), and visual-spatial (VS). When the
191 WM task was temporal, participants were instructed to remember the pattern of inter-stimulus
192 intervals (i.e., the rhythm), regardless of spatial locations. When the WM task domain was spatial,
193 participants had to remember the locations of the stimuli, regardless of order or timing (Fig. 1C).
194 In all but the AS WM task (see below), both the locations and intervals could change between the
195 encoding and probe sequences, but participants were instructed to ignore changes in the unattended
196 domain.

197 Participants retained stimulus information in WM for 5.5 seconds, after which a four-
198 stimulus probe sequence was presented in the same sensory modality as the encoded sequence.

199 Participants compared the encoded and probe sequences and made a same-different judgment on
200 the remembered domain (temporal or spatial). After the conclusion of the probe stimulus,
201 participants had 1.5 sec to indicate whether the encoded and probe sequences were the same (by
202 pressing “1” on the keyboard) or different (by pressing “0”). Each block contained an equal number
203 of same and different trials, ordered randomly. Participants maintained fixation on a small black
204 cross (0.41° visual angle) at the center of the display throughout the trial.

205 Pilot testing with earlier versions of these WM tasks revealed necessary adjustments to
206 prevent ceiling or floor effects in some conditions. For participants to perceive the different inter-
207 stimulus intervals equally well, a larger separation was needed for the visual stimuli (200 and 580
208 ms) than the auditory stimuli (200 and 340 ms). Conversely, the visual-spatial task was too easy
209 with only five stimulus locations, so the number of potential visual locations was increased to 12.
210 Finally, participants struggled to perform the AS WM task when stimulus timing was variable;
211 therefore, both encoding and probe stimuli in this condition were presented isochronously at the
212 longer inter-stimulus interval.

213 On some trials, participants also performed an Intervening task during the WM retention
214 period. This task was always auditory to allow pupil diameter to be measured in the absence of
215 any visual stimulation, but like the WM tasks, it could be either temporal or spatial (AT or AS; see
216 Fig. 1D). The stimulus structure was the same for the temporal and spatial variants. Starting 2 sec
217 after the offset of the final stimulus in the WM encoding phase, a sequence of three auditory stimuli
218 was presented. These stimuli were white noise bursts, acoustically distinct from the stimuli used
219 in the auditory WM tasks (tone complexes). One of the two intervals between the stimuli was
220 randomly chosen to be slightly longer than the other. The precise intervals were jittered on each
221 trial, with an average interval duration of 460 ms and a 90 ms average difference between the two

222 intervals. The sounds were presented from the two near-frontal loudspeakers (-4° and 0° azimuth).
223 The first stimulus played from one of these loudspeakers, chosen randomly and with equal
224 probability; the second stimulus was played from the other loudspeaker, and the third was played
225 from the same location as the first. In the temporal Intervening task, participants judged whether
226 the first or second inter-stimulus interval was longer. In the spatial Intervening task, participants
227 were asked to determine whether the second sound was to the left or right relative to the first and
228 third sounds.

229 This stimulus design allowed physically identically auditory stimuli to be used for the
230 spatial and temporal Intervening task conditions. However, it did introduce an asymmetry between
231 conditions in the amount of information required to do the task. In the temporal Intervening task,
232 participants needed to attend all three stimuli in order to compare the two inter-stimulus intervals,
233 whereas in the spatial Intervening task, participants were often able to make their judgment by the
234 second auditory stimulus by comparing its location to the first. This could result in a longer period
235 of increasing pupil size in the temporal task, leading to larger peak pupil diameter. However, our
236 analyses are primarily focused on comparing the four WM conditions *within* each Intervening task,
237 as behavioral accuracy was unequal between the two tasks. By deemphasizing across-task
238 comparisons, we sought to minimize the impact that potential differences in behavioral strategy
239 could have on our main conclusions.

240 Participants registered Intervening task responses with a keypress immediately after the
241 last Intervening task stimulus. Thus, neural signatures of motor planning and execution may be
242 present in the EEG data near the end of the WM retention phase. However, we deemed this less
243 detrimental than asking participants to hold their Intervening task responses until the end of the
244 trial, as such a design would increase the WM load in trials with an Intervening task and obfuscate

245 comparison with the no Intervening task conditions. Furthermore, any motor components in the
246 EEG data should be present whenever there was an Intervening task, allowing for fair comparison
247 between the different combinations of WM and Intervening tasks.

248 Trials were grouped into blocks of 20, with the WM and (if present) Intervening task
249 conditions held constant throughout the block. At the start of each block, an instruction screen
250 indicated the sensory modality and relevant domain (temporal or spatial) of the upcoming trials.
251 Participants were allowed to take untimed breaks between blocks. Participants performed one
252 block of each WM and Intervening task combination before any conditions were repeated, and the
253 same condition was not allowed to repeat in adjacent blocks. In total, participants performed 40
254 trials of each combination of WM task modality, WM task domain, and Intervening task condition.

255 Each complete dataset required three separate visits to the lab. The first session was
256 reserved for consent, subject screening, and task practice. Participants practiced each variant of
257 the WM and Intervening tasks in isolation until they understood the procedure, then three to five
258 example trials of the full dual-task paradigm. Data collection for the actual experiment occurred
259 in the two subsequent sessions, which were split based on the sensory modality of the WM tasks;
260 auditory and visual WM tasks were performed on separate days. Session order was randomized
261 and counterbalanced across participants.

262

263 *Stimulus Details*

264 For the visual WM tasks, 12 stimuli were arranged in a circle centered on the fixation cross
265 and shown on a constant dark grey background (2.51 cd/m^2). Each stimulus was a square patch of
266 visual noise, subtending 2.86° of visual angle and composed of a 30×30 grid of smaller squares.
267 Each of these smaller squares was filled with a greyscale color between black and white, such that

268 the average luminance across the patch was 5.85 cd/m². The angular spacing between each patch
269 was 30°, and the entire stimulus circle subtended 21.59° of visual angle. To equate display
270 luminance and structure across tasks, these visual stimuli remained present but static throughout
271 the auditory WM and Intervening tasks. To employ these stimuli in the visual WM tasks, the
272 luminance of each small square in a given patch could be resampled; this made the visual patch
273 appear to jitter without changing the average luminance across the patch.

274 For the auditory WM tasks, each stimulus was a 50-ms tonal chord consisting of 3
275 harmonically unrelated complex tones (fundamental frequencies of 422, 563, and 670 Hz); each
276 complex was made up of its first nine harmonics with equal amplitude. The same tone complex
277 was used for all auditory stimuli in the WM tasks. WM task stimuli were only presented from the
278 loudspeakers at ±90°, ±45°, and 0° azimuth. For the Intervening tasks, which were always auditory,
279 the stimuli were one of five pre-generated, 50-ms bursts of noise bandpass filtered between 100
280 and 10,000 Hz. Identical noise tokens were used for all three stimuli within each Intervening task
281 sequence. These WM and Intervening task stimuli were chosen to be distinct, such that stimuli
282 were clearly different between the two tasks. Both types of stimuli were relatively broadband, thus
283 ensuring they provided rich and robust spatial localization cues. All auditory stimuli were ramped
284 on and off with a 5 ms cosine-squared ramp to avoid spectral splatter and transient onset and offset
285 artifacts.

286 In the visual WM tasks, the first stimulus to change in the encoding and probe sequences
287 was always the one at top-center (12 o'clock). Similarly, in all auditory WM sequences, the first
288 sound was presented from the central loudspeaker. This was done to equate the number of items
289 stored in WM across the spatial and temporal WM tasks. With four stimuli in each sequence, there

290 were three intervals to remember for the temporal tasks, and so the first stimulus location was held
291 constant such that only three locations needed to be remembered for the spatial tasks.

292

293 *Behavioral Data Analysis*

294 The primary behavioral metrics in this study were the error rates on the WM and
295 Intervening tasks. Reaction time estimates could not be made because 1) the position in the probe
296 sequence at which a decision could be made differed based on whether the correct response was a
297 “same” (final stimulus) or “different” (often earlier); and 2) within “different” trials, any of the
298 second, third, or fourth stimuli could contain the change.

299 Statistical outcomes of behavioral performance were analyzed using logistic mixed effects
300 regression models. For the WM task, the model included fixed effect terms for WM task modality,
301 WM task domain, and Intervening task, and random effects terms to capture participant-specific
302 intercepts for all three predictor variables. In Wilkinson notation, the model was specified as:

$$303 \quad \text{logit}(\text{Error Rate}) \sim \text{Modality}_{WM} * \text{Domain}_{WM} * \text{Int} \\ 304 \quad \quad \quad + (1 + \text{Modality}_{WM} + \text{Domain}_{WM} + \text{Int} | ID)$$

305 Due to the fundamental differences between the four WM conditions, differences in retrieval
306 between these conditions were not of primary interest. Instead, we focused post-hoc analyses on
307 how retrieval in each WM condition was impacted by modality and domain similarity with the
308 Intervening task. To this end, post-hoc comparisons were only conducted within each WM task
309 condition (e.g., examining differences in AT WM retrieval between the AT, AS, and No
310 Intervening task conditions). Similarly, for Intervening task performance, we held the Intervening
311 task fixed and compared error rates between the four WM task conditions. This analysis required
312 us to compare across levels of both WM modality and WM domain; to facilitate this, the

313 Intervening task model was constructed with these factors collapsed into a single predictor
314 variable, WM Condition:

$$315 \quad \text{logit}(\text{Error Rate}) \sim \text{WM Condition} * \text{Int} + (1 + \text{WM Condition} + \text{Int} | \text{ID})$$

316 To investigate main effects and interactions at the group level, the coefficients from these
317 models were supplied to a 3-way (WM task) or a 2-way (Intervening task) repeated measures
318 ANOVA. Contrasts were initially treatment coded with base levels set as “auditory” for WM
319 modality, “temporal” for WM domain, and “none” for Intervening task – these choices had no
320 impact on the outcome of the group-level ANOVA. However, pairwise post-hoc testing was
321 conducted by cycling which level was considered “baseline” for each factor until a β weight (and
322 corresponding p-value) could be extracted for each necessary pair of levels. All post-hoc tests were
323 Bonferroni-Holm corrected for multiple comparisons.

324

325 *Pupillometry data collection and analysis*

326 Both pupils were tracked with a combination of the corneal reflection and a fit of the pupil
327 border using SR Research algorithms. Prior to the start of each experimental session, eye position
328 measurements were calibrated based on five fixation points (display center, $\pm 20^\circ$ azimuth on the
329 horizontal plane, and $\pm 10^\circ$ elevation on the median plane). This calibration was validated at the
330 center position prior to each trial, and at all five points at the start of each block. Whenever eye
331 position was offset from the calibration by an average of greater than 4° , the full five-point
332 calibration was repeated. The experimenter monitored gaze position throughout the experiment; if
333 at any point during the trial the participant’s gaze deviated substantially from 0° in either azimuth
334 or elevation, the experimenter immediately stepped in to ensure that the participant maintained
335 center fixation moving forward.

336 A custom MATLAB analysis pipeline and wrapper GUI were used to prepare pupil data
337 for statistical analysis. First, trials were split into baseline and trial windows, where the trial
338 window spanned the start of the WM encoding sequence through the end of the WM retention
339 phase. Next, blinks were automatically detected based on instantaneous position, velocity, and
340 acceleration thresholds. An experimenter manually reviewed the data, and using the GUI, adjusted
341 blink thresholds or manually marked additional blink segments as needed. Blinks and other marked
342 segments of noisy data were replaced with a linear interpolation between the average of the three
343 samples preceding and following the blink. When blinks occurred at the beginning of the trial
344 window, a linear fit was made to the five samples following the blink, and this fit was back-
345 projected through the blink segment. The opposite procedure was used for blinks falling at the end
346 of the trial window. Trials in which more than 25% of the data was made up of rejected segments
347 were automatically excluded from further analysis. When data from both eyes were available, the
348 two traces were averaged. To produce the final output, the traces were concatenated, Z-scored,
349 then split back into trials and trial windows. This procedure eschewed absolute pupil size measures
350 in favor of values that were individually normalized for each participant, so only relative pupil
351 diameter between conditions is interpreted.

352 Statistical testing for differences between conditions in the pupil time courses was carried
353 out using non-parametric permutation tests. First, at each time point, the difference between two
354 conditions was assessed parametrically using a paired T-test across the individual participant
355 average data. Next, 2000 iterations of randomly shuffling the condition labels for each participant's
356 data were performed; these randomly labeled samples were used to recompute paired T-tests at
357 each time point, generating a null distribution of 2000 such values. Finally, at each time point, the
358 significance level of the actual difference was determined by calculating the percentage of the null

359 distribution with a T-value equal to or larger than the T-value from the actual data. Significant
360 differences were only considered reliable if the p-value fell below 0.05 for a minimum of 15
361 consecutive samples.

362

363 *EEG Data Analysis*

364 EEG analyses were carried out using the FieldTrip package in MATLAB (Oostenveld et
365 al., 2011). For event-related potential (ERP) analyses, EEG preprocessing comprised the following
366 steps: read in the continuous data one channel at a time and immediately downsample to 256 Hz;
367 re-reference the data to the average of two electrodes placed on the mastoids, bandpass filter
368 between 0.5 and 20 Hz (zero-phase FIR filter, transition width of 0.2 Hz, order of 9274); manually
369 identify and remove segments containing muscle artifacts; perform an independent components
370 analysis (ICA) to project out blinks and saccadic eye movements; epoch the data from 100 ms
371 before to 500 ms after each individual auditory or visual stimulus (timing differences precluded
372 whole-trial averaging); reject any epochs in which the data exceeded a 100 μ V peak-to-peak
373 threshold; and baseline correct by subtracting off the mean of the first 100 ms of each epoch.

374 For time-frequency analyses, a similar preprocessing pipeline was used, but with a few key
375 differences. First, the low-pass filter cutoff was raised to 80 Hz. Second, participant average ERPs
376 (recomputed with the new filter cutoffs) were subtracted from the data in the time domain
377 immediately prior to epoching; this step served to minimize phase-locked evoked contributions to
378 the time-frequency response. Subtracted ERPs were specific to each trial phase (i.e. encoding,
379 retention, and probe), WM and Intervening task condition, and position in the stimulus sequence.
380 Third, the data was split into whole-trial epochs, spanning the baseline period through the final
381 stimulus in the probe sequence, instead of shorter individual stimulus epochs. The continuous

382 Morlet wavelet transform (wavelet width of 5 cycles in 1 Hz steps) was used to obtain the power
383 spectra of each trial. Prior to wavelet analysis, the signal was padded to avoid edge artifacts. This
384 was done by copying the first and last 5 seconds of the epoch, reflecting each copy on the time
385 axis, then appending them to the beginning and end of the signal, respectively. Finally, the data
386 was split into the three key trial phases: WM encoding, WM retention/Intervening task, and WM
387 probe.

388 We extracted time courses from the resulting power spectra at each channel in the theta (4-
389 8 Hz) and alpha (8-13 Hz) frequency bands. To produce theta time courses, power estimates
390 centered on 4, 5, 6, and 7 Hz (1 Hz bandwidth) were averaged for each participant. Individual
391 differences in the peak frequency of alpha oscillations are well-established (Klimesch et al., 1999).
392 Thus, for alpha time courses, the individual alpha frequency for each participant was defined as
393 the frequency at which the absolute value of the alpha change relative to baseline was maximal
394 during WM retention (the direction of alpha change was found to flip based on WM modality in
395 the present study). Alpha power time courses were reported as the power at this frequency averaged
396 with the power 1 Hz above and below the individually defined alpha frequency.

397 Similar to the pupillometry data, EEG data were analyzed using non-parametric
398 permutation testing, this time implemented using FieldTrip software. To control the multiple
399 comparisons problem with high-dimensional EEG data, we used cluster-based permutation testing
400 to analyze ERPs and oscillatory power time courses. Paired t-tests were first conducted at each
401 time-channel data point. Those comparisons reaching a significance threshold (generally $p < 0.01$)
402 were grouped into clusters of points contiguous in time and within 40 mm scalp distance of one
403 another. The “mass” of this cluster was then computed as the sum of T-scores across all member

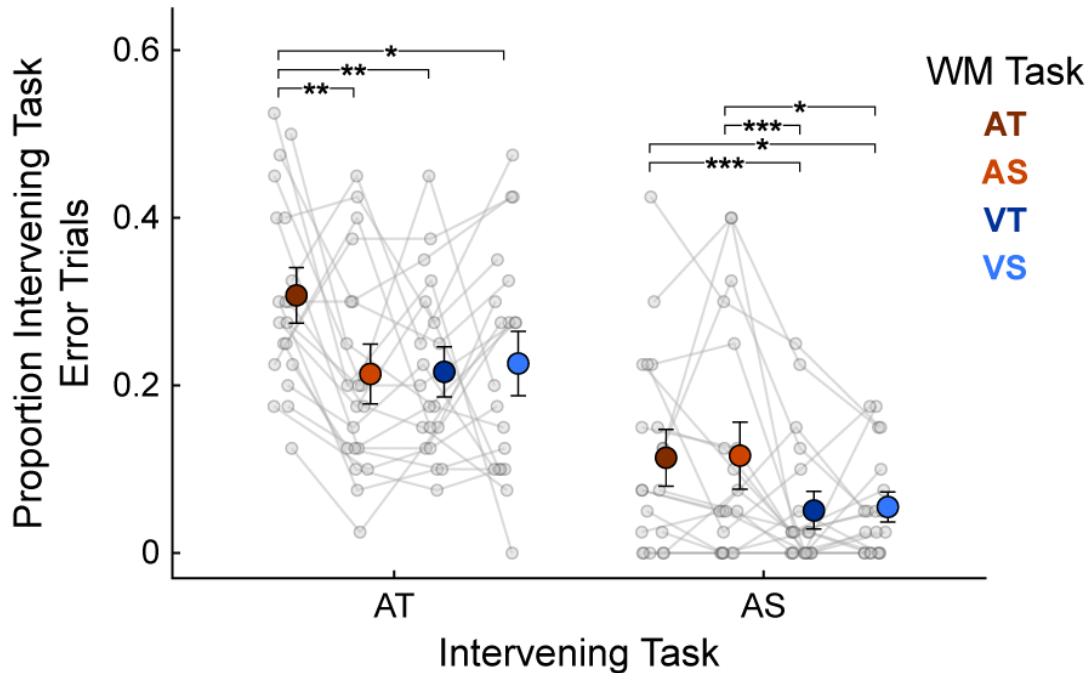
404 points. Finally, this cluster mass was compared against a null distribution of clusters formed by
405 2000 random permutations of the condition labels.

406

407 **Results**

408 *Intervening Task Performance*

409 Performance accuracy on the Intervening tasks depended on both the Intervening task
410 condition and the modality and domain of the information participants were holding in WM (Fig.
411 2). These effects were analyzed using a logistic mixed-effects model with fixed-effect terms of
412 Intervening task (AT or AS) and WM task (AT, AS, VT, or VS). Random-effects terms included
413 by-participant intercepts for both fixed effects. Group-level significance of the fixed effects and
414 their interaction were tested in a Type-III ANOVA, with p-values based on the Satterthwaite
415 approximation for degrees of freedom. This ANOVA revealed significant main effects of
416 Intervening task ($\chi^2 = 32.7$, $df = 1$, $p = 1.07 \cdot 10^{-8}$) and WM task ($\chi^2 = 17.6$, $df = 3$, $p = 5.29 \cdot 10^{-4}$),
417 as well as a significant interaction between these factors ($\chi^2 = 24.1$, $df = 3$, $p = 2.44 \cdot 10^{-5}$). The
418 main effect of Intervening task indicates that performance was better overall on the AS Intervening
419 task than the AT Intervening task. This difference simply reflects a limit on the difficulty of the
420 AS Intervening task imposed by how close together the two loudspeakers could be placed. Since
421 performance differed widely between the two Intervening tasks, we focused pairwise post-hoc
422 tests on conditions in which the Intervening task was the same; differences between these
423 conditions could only be caused by the type of information participants were holding in WM.



424

425 **Figure 2: Intervening task error rates for each combination of WM task and Intervening task.** Grey
426 points represent individual participants, colored circles represent means, and error bars represent S.E.M.
427 Chance performance is at an error trial proportion of 0.5. Asterisks indicate significant contrasts between
428 WM task levels in the mixed-effects model, which were examined separately within each Intervening task.
429 * = $p < 0.05$, ** = $p < 0.01$, *** = $p < 0.001$ after Bonferroni-Holm correction.
430

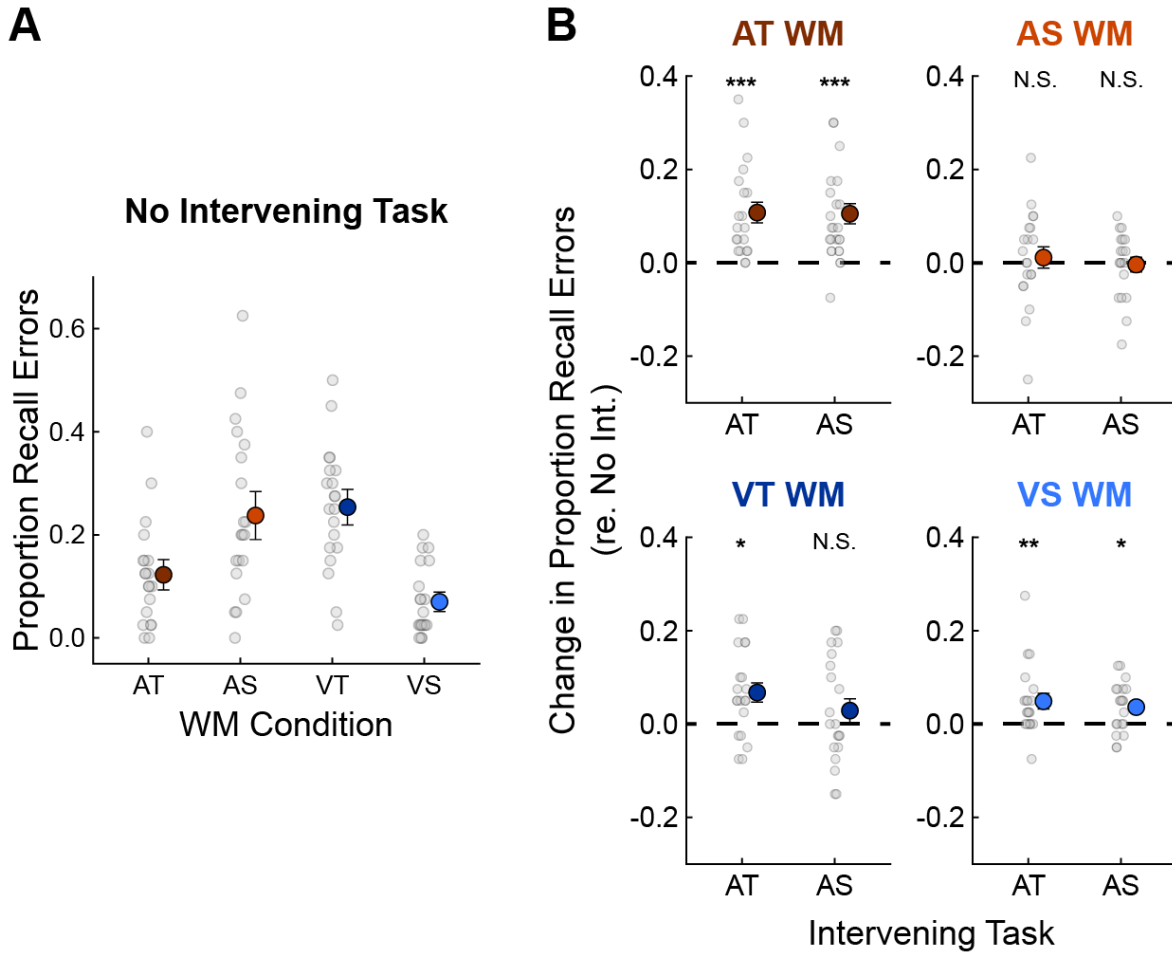
431 As a means of post-hoc testing, we report the significance of contrasts in the mixed-effects
432 model coding for each pair of WM tasks, with p-values adjusted for multiple comparisons using
433 the Bonferroni-Holm correction. Participants made significantly more errors on the AT
434 Intervening task when the information being held in WM was also AT, as compared to all the other
435 WM conditions (AT vs. AS, $p = 0.006$; AT vs. VT, $p = 0.003$; AT vs. VS, $p = 0.03$; Fig. 2, left).
436 Accuracy on the AS Intervening task appeared to depend primarily on the sensory modality of the
437 WM task, with participants making significantly more errors when both tasks were auditory than
438 when the WM task was visual (AT vs. VT, $p = 1.76 \cdot 10^{-5}$; AT vs. VS, $p = 0.026$; AS vs. VT, $p =$
439 $5.50 \cdot 10^{-5}$; AS vs. VS, $p = 0.021$; Fig. 2, right). Note that error rate floor effects were apparent on
440 the AS Intervening task, which may have limited our ability to detect additional interference effects

441 based on WM domain. Nonetheless, participants generally committed more errors on the
442 Intervening task when it matched the modality – and in the case of the AT Intervening task, the
443 domain – of the information stored in WM.

444

445 *Working Memory Task Performance*

446 Participants were able to retrieve the information stored in WM at better-than-chance levels
447 across all combinations of WM modality, WM domain, and Intervening task (Fig. 3). These factors
448 (including conditions with no Intervening task) were included as fixed effects in a logistic mixed
449 effects model of WM task retrieval errors. Random-effects terms included by-participant intercepts
450 for all fixed effects, and group-level significance of the fixed effects was again tested using a Type-
451 III ANOVA. This ANOVA revealed a significant interaction between WM task modality and
452 domain ($\chi^2 = 206.4$, $df = 1$, $p < 10^{-15}$), reflecting overall lower error rates on the AT and VS WM
453 tasks, in which the sensory modality was optimally suited for the information domain of the task
454 (Fig. 3A). The ANOVA also revealed a three-way interaction between WM modality, WM
455 domain, and Intervening task ($\chi^2 = 19.0$, $df = 2$, $p = 7.66 \cdot 10^{-5}$), indicating differential effects of the
456 Intervening tasks depending on WM condition. These effects were explored via post-hoc testing,
457 again restricted to conditions in which the task being measured – in this case, the WM task – was
458 the same, with differences in WM retrieval now attributable only to the Intervening task type.



459
460 **Figure 0: Working memory task performance.** A, The proportion of trials on which the WM information
461 was retrieved incorrectly is plotted for conditions without an Intervening task. Chance performance is at
462 0.5. B, The change in retrieval error rate is plotted for each WM and Intervening task combination relative
463 to the no Intervening task conditions. The dashed line at 0 indicates no change in WM retrieval. Post-hoc
464 comparisons were limited to differences between Intervening task conditions within each WM task.
465 Asterisks indicate significant differences from the corresponding no Intervening task conditions (no
466 significant differences were found between the two Intervening tasks). * = $p < 0.05$, ** = $p < 0.01$, *** = p
467 < 0.001 after Bonferroni-Holm correction.

468

469 To visualize effects of the Intervening tasks on WM task accuracy, Fig. 3B shows the
470 difference between error rates when an AT or AS Intervening task was present and the
471 corresponding condition with no Intervening task. When the WM task was AT, both of the auditory
472 Intervening tasks significantly impaired WM retrieval ($p < 10^{-6}$ for both; top-left panel of Fig. 3B).
473 When the WM task was AS, on the other hand, the Intervening tasks had no detectable impact on

474 WM retrieval (top-right panel). We suspect that retaining AT information in WM relied solely on
475 the auditory-temporal WM network, leading to memory interference from the auditory Intervening
476 tasks. In the AS WM task, on the other hand, sound locations to be remembered were likely
477 mapped into a representation in the visual-spatial WM network, protecting this information from
478 auditory interference.

479 The fact that accuracy on the AS WM task was relatively poor might have impaired our
480 ability to detect effects of the Intervening tasks in this condition, as retrieval was closer to chance
481 before the Intervening task was added (Fig. 3A). To explore this possibility, we performed a
482 median split of the AS WM task data in the no Intervening task condition, then tested for
483 differences in the effects of the Intervening tasks between the better and worse performing
484 participants. One might expect that the Intervening tasks would impair retrieval only among the
485 better performers; this group started further from chance performance, resulting in more room for
486 their performance to be affected by the Intervening tasks. However, this was not the case; neither
487 Intervening task significantly altered AS WM task performance for either the better or worse
488 performers, and the effects of the Intervening tasks did not differ between the two groups
489 (uncorrected paired T-tests, all p-values > 0.27).

490 In some cases, visual WM retrieval was also modestly impaired by the auditory Intervening
491 tasks. A small but significant increase in retrieval errors on the VT WM task was detected when
492 the Intervening task was also temporal ($p = 0.042$; bottom-left panel of Fig. 3.6B). This might
493 reflect domain-based WM interference with both tasks drawing on an auditory-temporal network,
494 although no significant difference was found between the AT and AS Intervening task conditions.
495 In the VS WM condition, both Intervening tasks increased retrieval errors ($p = 0.003$ for AT
496 Intervening task, $p = 0.044$ for AS; bottom-right panel). This result was surprising given the lack

497 of modality or domain similarity between the WM and Intervening tasks. However, in this case
498 the errors may reflect a task-switching cost as participants shifted from performing an auditory
499 perceptual judgment to retrieving visual-spatial information from WM.

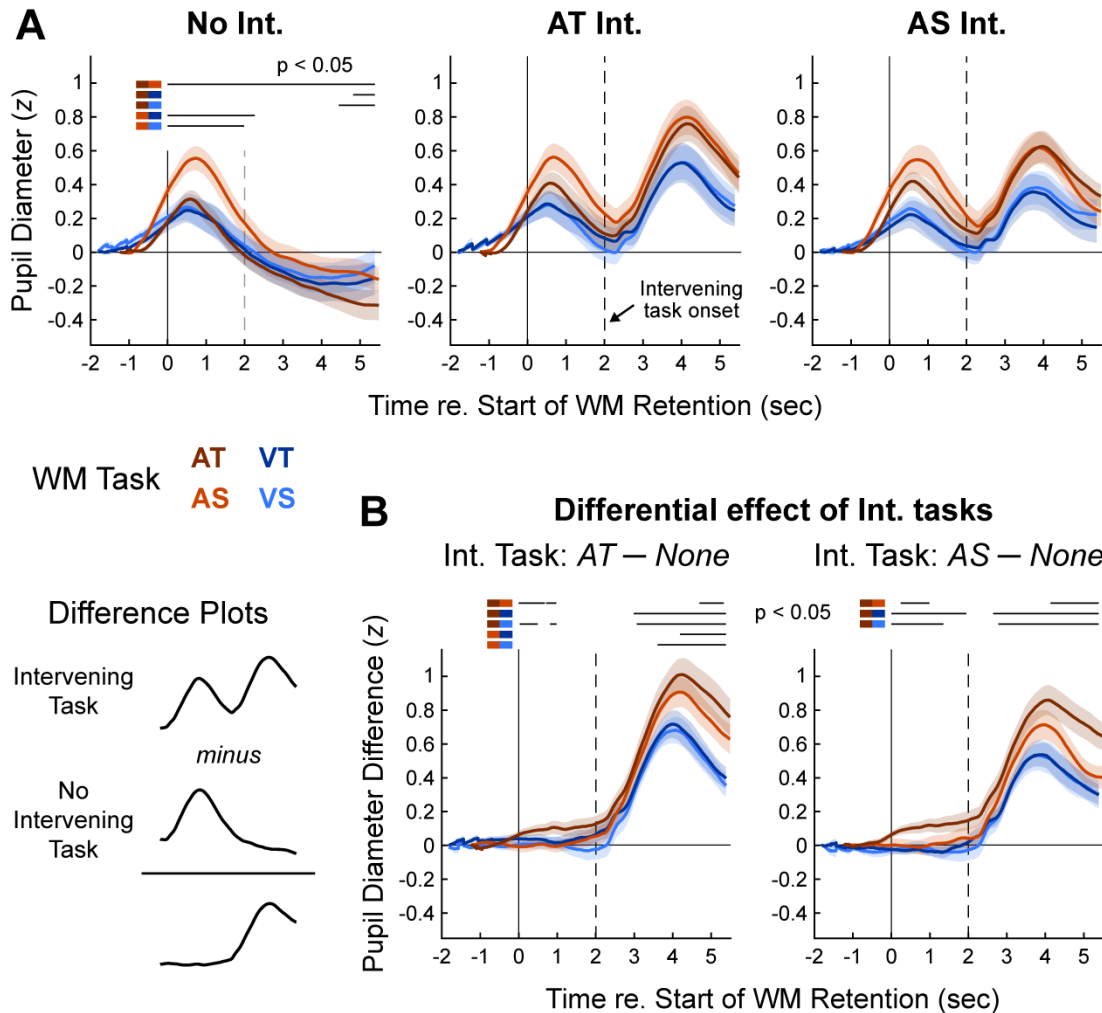
500

501 *Pupil Dilations*

502 Encoding information in WM and performing the auditory Intervening tasks both led to
503 reliable pupil dilations, shown in Fig. 4. In the absence of an Intervening task, pupil diameter
504 increased throughout presentation of the stimuli to be encoded in WM (negative values on the time
505 axis), peaked about 700 ms after the final WM encoding stimulus (time zero), and then gradually
506 declined throughout WM retention (Fig. 4A, left panel). The onset of the AT and AS Intervening
507 tasks (at 2 sec on the time axis) produced large secondary dilations, the amplitude of which was
508 modulated by the information participants were holding in WM (Fig. 4A, middle and right panels).

509 Statistical differences between the pupil responses were assessed using non-parametric
510 permutation testing, restricted to a time window spanning the WM retention phase (time zero and
511 later). Tests was not conducted during WM task stimulus presentation because 1) the traces were
512 baseline-corrected to zero at the start of this window, and 2) the interstimulus-intervals differed
513 between auditory and visual WM conditions (see Methods), leading to different trace durations. In
514 the absence of an Intervening task, AS WM encoding elicited a markedly larger pupil response
515 than any of the other WM conditions (Fig. 3A). This may have reflected the generally higher
516 difficulty of the AS WM task as compared to the AT WM task. However, while a similar
517 performance difference was found between the VT and VS conditions, no difference in pupil
518 dilations was detected between these conditions. Thus, these results may suggest an asymmetry

519 between the cognitive costs of encoding auditory information into a visual-spatial framework (AS
 520 WM) and encoding visual information into an auditory-temporal representation (VT WM).
 521



522 **Figure 4: Pupillometry results.** **A**, Grand average z-scored pupil responses in the No Intervening task
 523 condition (left) and elicited by physically identical stimuli in the AT (middle) and AS (right) Intervening
 524 tasks. Solid vertical lines represent the end of WM encoding and the start of WM retention, while dashed
 525 vertical lines indicate the onset of the Intervening task. Error clouds represent S.E.M. Horizontal black lines
 526 above the traces represent time regions of significant difference in permutation testing, with the two WM
 527 conditions being compared indicated by colors next to each significance line. **B**, The difference between
 528 pupil responses elicited in conditions with an Intervening task and responses in the corresponding WM
 529 conditions with no Intervening task.
 530
 531

532 Pupil dilations elicited by both auditory Intervening tasks were larger when the information
533 stored in WM was auditory than when it was visual, mirroring the modality-driven interference
534 effects observed in the behavioral data (Fig. 4A, middle and right panels). To more clearly separate
535 the differential impact of the Intervening tasks on pupil diameter, we subtracted corresponding
536 pupil traces with no Intervening task from each pupil trace with an Intervening task (Fig. 4B). As
537 a preliminary analysis, we averaged these residual pupil traces across WM conditions and tested
538 for a difference between the two Intervening tasks. This confirmed that traces elicited by the AT
539 Intervening task were larger overall than those elicited by the AS Intervening task ($p < 0.05$ for all
540 time points between 3.7 sec after WM retention onset and the end of the WM retention window;
541 not shown), matching the higher behavioral error rates on the AT task.

542 Next, we compared the residual pupil traces between the four WM conditions within each
543 Intervening task, similar to our treatment of the Intervening task behavioral data. Differential pupil
544 dilations elicited by both Intervening tasks were larger when the information held in WM was
545 auditory than when it was visual, as can also be observed in the raw traces in Fig. 4A. However,
546 expressing the pupil dilations relative to conditions without an Intervening task revealed the largest
547 differential response when the WM task was AT – significantly larger than when the WM task was
548 AS – for both Intervening tasks. Further, the residual pupil traces were elevated prior to Intervening
549 task onset in the AT WM condition, indicating larger pupil dilations during WM encoding when
550 an Intervening task was upcoming. This suggests a preparatory modulation of task effort, with the
551 AT WM information needing to be encoded with particularly high fidelity in order to survive
552 interference from an auditory Intervening task. These results are broadly consistent with the
553 behavioral data, in which the auditory Intervening tasks tended to be most costly when the WM
554 task was AT. We expect that the AT WM condition maximally loaded auditory-biased attention

555 and WM networks, which were also necessary to process the stimuli in either of the auditory
556 Intervening tasks.

557 In the visual WM conditions, pupil dilations were insensitive to whether the WM task was
558 temporal or spatial. This result mirrors the behavioral data and indicates that interference was
559 generally low when the two tasks were presented in different sensory modalities, even if they were
560 matched in information domain. Importantly, the patterns of pupil dilations we observed cannot
561 readily be explained by differences in WM task difficulty. Average pupil dilations were larger with
562 auditory than visual information held in WM, particularly when the WM task was AT. A pure
563 difficulty-based account would therefore predict that WM retrieval should be worst in the AT
564 condition, when in fact participants performed worst on the AS and VT WM tasks, in which the
565 sensory modality was sub-optimal for the information domain of the task. Instead, the pupil
566 dilations observed here likely reflect patterns of dual-task interference specific to the similarity in
567 modality and domain between the two tasks.

568

569 *Event-related potential (ERP) amplitudes*

570 While the behavioral and pupillometry data revealed consistent effects of the modality and
571 domain of the WM task, the domain of the Intervening task had relatively little impact on the
572 pattern of dual-task interference. One explanation for this could be that the AS Intervening task
573 did not recruit the visual-spatial attention network to the same extent as the AS WM task. The AS
574 Intervening task required only an immediate, relative judgement about sound locations, whereas
575 the AS WM task required participants to remember absolute sound positions by placing them in
576 allocentric reference frame. Thus, both Intervening tasks may have predominantly loaded on the
577 auditory-temporal attention network, resulting in similar behavioral and autonomic signatures of

578 interference. Nonetheless, the AT and AS Intervening tasks did require different types of auditory
579 processing, which could affect patterns of dual-task interference at the neural level; we next
580 investigated this possibility in the EEG data.

581 We first examined event-related potentials (ERPs) elicited by stimulus events in the WM
582 and Intervening tasks. Grand average ERPs elicited by each stimulus event can be seen in
583 Supplemental Fig. 1. ERPs elicited by stimuli in the encoding and probe sequences of the WM
584 task were not systematically modulated by the Intervening tasks. However, ERPs elicited by the
585 Intervening task stimuli – particularly the first sound in the Intervening task sequence – were
586 modulated by the information participants were holding in WM. Unlike ERPs elicited by the
587 auditory WM tasks, the Intervening task ERPs had a somewhat atypical morphology, including
588 weak N1 and strong P2 components. This may have been due to the acoustic differences between
589 the WM and Intervening task stimuli, or modulation of ERP morphology due to the fact that
590 participants were holding information in WM. Regardless, both the modality and domain of the
591 information in WM affected the amplitude of the P2 component of the Intervening task onset ERPs
592 (Fig. 5, panels A and B). To quantify these effects, P2 amplitudes were calculated for each
593 participant as the average of the ERP waveform between 170 and 230 ms post-stimulus across a
594 cluster of fronto-central electrode sites (Fz, FCz, Cz, FC1, and FC2 on the standard 10-20 layout).
595 These P2 amplitudes were then modeled using a 3-way ANOVA with explanatory factors of WM
596 modality, WM domain, and Intervening task. This analysis revealed a significant main effect of
597 WM modality ($F = 7.27$, $df = 1$, $p = 0.014$) and a significant interaction between WM domain and
598 Intervening task ($F = 10.83$, $df = 1$, $p = 0.004$), both of which will be examined in more detail
599 below.

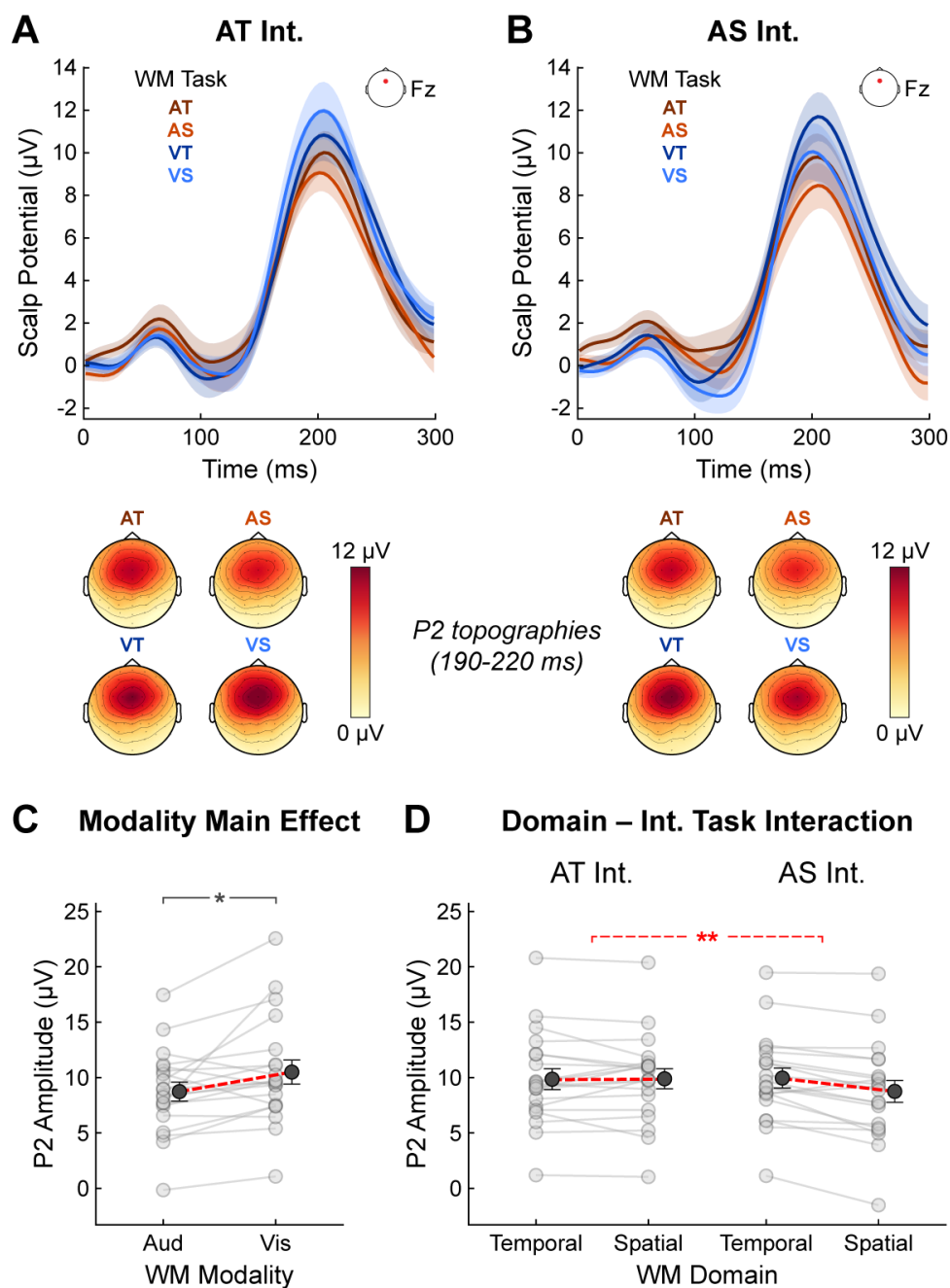


Figure 2: ERP results. **A**, Grand average ERPs elicited by the onset of the AT Intervening task at a fronto-central electrode site (Fz). Color represents the WM task, and error clouds represent S.E.M. Scalp topographies of the P2 responses are shown below the traces. **B**, Same as A, but for the AS Intervening task. **C**, P2 peaks as a function of WM modality, averaged across WM domain and Intervening task. **D**, P2 peaks averaged across WM modality to illustrate the significant interaction between WM domain and Intervening task.

600

601

602 Starting with the main effect of WM modality, the amplitudes of P2 components elicited
603 by both auditory Intervening tasks were larger when *visual* information was stored in WM than
604 when the WM task was auditory (Fig. 5C). This could reflect a greater availability of auditory
605 processing resources to respond to the Intervening task stimuli when these resources had not
606 previously been taxed by an auditory WM task. An alternative explanation is that the auditory
607 stimuli in the WM task caused habituation of the auditory Intervening task ERPs, resulting in
608 suppressed P2 amplitudes. While the 2-second gap between WM encoding offset and Intervening
609 task onset is close enough to reduce ERP amplitudes (Budd et al., 1998), such habituation would
610 likely have been reset by the acoustic differences between the WM and Intervening task stimuli,
611 similar to what occurs during auditory oddball paradigms (Paavilainen, 2013). In addition, ERPs
612 elicited by the *final* AT Intervening task stimuli were modulated in a similar fashion to the onset
613 ERPs (see Supplemental Fig. 1), which is inconsistent with a simple habituation account. A similar
614 modulation of the final Intervening task ERPs was not observed in the AS task, but in this task,
615 participants could sometimes make their decision before the final stimulus by comparing the first
616 and second stimulus locations. Thus, the observed modulation of P2 amplitudes likely reflects
617 resource availability for Intervening task processing, rather than auditory response habituation.

618 P2 amplitudes were also affected by domain similarity between the tasks, as evidenced by
619 the significant interaction between WM domain and Intervening task. Specifically, P2s elicited by
620 the first AS Intervening task stimulus were suppressed when the WM task was also spatial; this
621 effect was, on average, smaller for the AT Intervening task (Fig. 5D). Although the three-way
622 interaction involving WM task modality did not reach statistical significance, the two-way
623 interaction appears to have been driven by the visual WM conditions, in which P2s were larger
624 when the domain differed between the two tasks. To demonstrate this, we split the P2 peak data

625 into auditory and visual WM conditions, then conducted separate 2-way ANOVAs with factors of
626 WM domain and Intervening task. The significant interaction between these terms remained in the
627 visual WM conditions ($F = 10.77$, $df = 19$, $p = 0.004$; beneath a Bonferroni-Holm adjusted alpha
628 criterion to account for the two additional ANOVAs, assuming an initial alpha criterion of $p =$
629 0.05). In the auditory WM conditions, no significant main effects or interactions were detected
630 (even when uncorrected for multiple comparisons). In sum, P2 components of the ERPs scaled
631 inversely with dual-task similarity in modality and domain. P2s amplitudes were generally higher
632 when the tasks were mismatched on either dimension, leading to the largest P2s when the tasks
633 differed in both modality and domain.

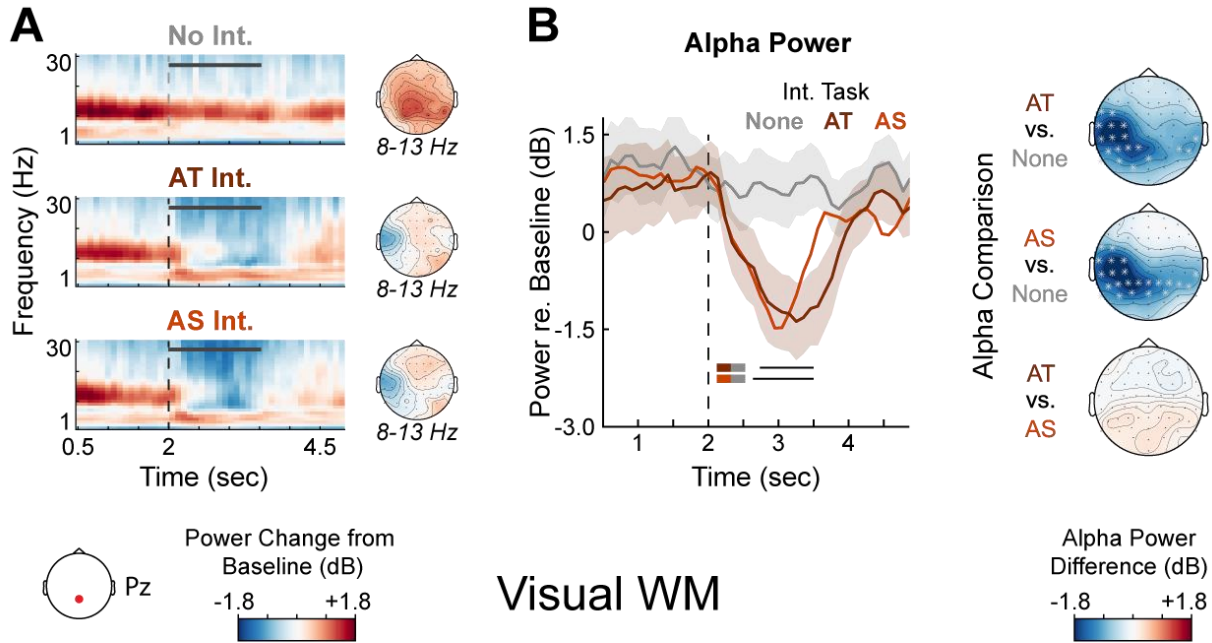
634

635 *Alpha-band oscillatory activity*

636 During WM encoding, oscillatory power in the alpha (8-13 Hz) frequency band steadily
637 increased relative to baseline in the auditory WM conditions, and decreased relative to baseline in
638 the visual WM conditions (Supplemental Fig. 2). These patterns of alpha power persisted into the
639 WM retention window, shown in Fig. 6. Preliminary analysis of alpha power in the retention
640 window using cluster-based permutation testing revealed no significant differences based on the
641 domain of the WM task, so data were collapsed across this dimension for the following analyses.
642 The grand average power spectrum during the pre-trial baseline, showing a clear peak in the alpha
643 band at a parietal electrode site, can be found in Supplemental Fig. 3.

644

Auditory WM



Visual WM

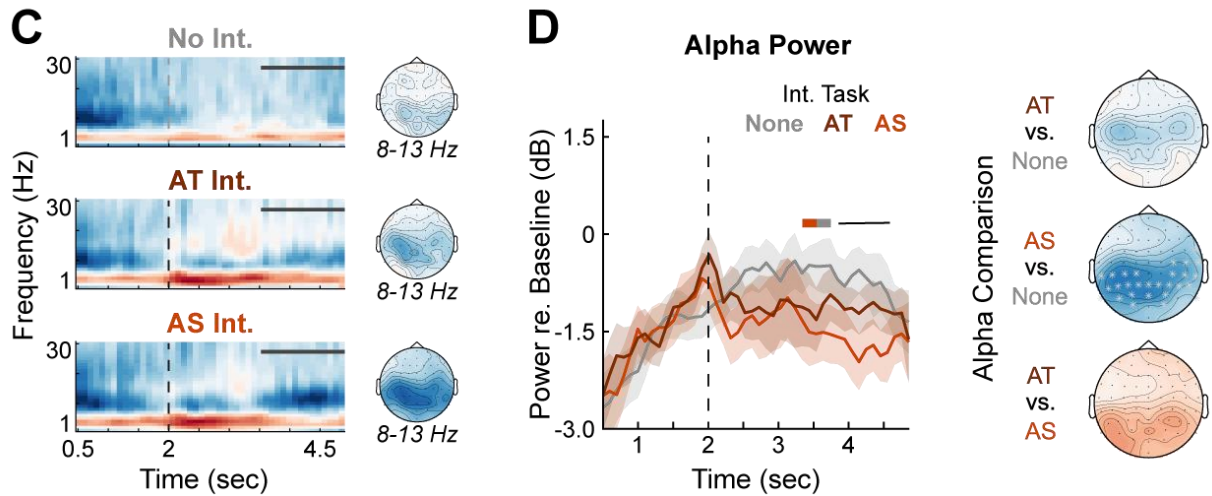


Figure 6: Alpha power results. Grand-average time-frequency responses are shown at a parietal electrode site (Pz) during the memory retention window for each of the three Intervening tasks and for auditory (**A**) and visual (**C**) WM. Responses are averaged across WM domain and shown as dB change relative to the average pre-trial baseline period across conditions. Vertical dashed lines represent Intervening task onset when present, and horizontal grey bars represent the time regions in which significant effects were found in cluster-based permutation testing. The first and last 500 ms of the retention window were excluded to limit power contributions from responses evoked by the WM task stimuli. A timing error in the experiment code shortened the memory retention window for two subjects by approximately 100 ms, and so all time-frequency responses were additionally truncated to match this shortened duration. **B**, Grand average alpha power time courses (left panels) and statistical comparisons (right panels) for the auditory WM conditions. **D**, Same as B, but for the visual WM conditions. Power time courses for each participant were calculated at their peak alpha frequency ± 1 Hz. Error clouds

646 represent S.E.M. Black horizontal bars indicate the temporal extent of significant clusters for the
647 comparisons shown in the topoplots to the right. When significant clusters were detected, the alpha power
648 difference was plotted only in the significant time region; otherwise, the topoplot time regions span the
649 entire cluster test window. * indicates channel membership in a significant cluster ($p < 0.05$).

650
651

652 In the auditory WM tasks, alpha power remained elevated relative to baseline throughout
653 the memory retention window when no Intervening task was present (Fig. 6A, top panel).
654 However, the onset of both the AT and AS Intervening tasks suppressed these ongoing alpha
655 oscillations (middle and bottom panels). We examined this effect by conducting cluster-based
656 permutation tests on the alpha power time courses (see Materials and Methods) in two time regions
657 of interest: one spanning the onset of the Intervening task through the end of the Intervening task
658 response window (2 to 3.5 seconds into WM retention), and another from 3.5 to 5 sec, during
659 which participants needed to start retrieving the information encoded in WM in anticipation of the
660 probe sequence. During both of the Intervening tasks (in the earlier window), alpha power was
661 significantly reduced relative to the no Intervening task condition (AT Intervening task, $p = 0.005$;
662 AS Intervening task, $p = 0.003$; Fig 6B). With the statistical threshold for generating the initial
663 clusters set at $p = 0.01$, no differences were found between alpha power in the two Intervening
664 tasks. However, relaxing this threshold to $p = 0.05$ revealed a late AT vs. AS Intervening task
665 cluster between 3.14 and 3.45 sec ($p = 0.026$; not shown). This indicates that the alpha power
666 reduction lasted longer when the Intervening task was AT than when it was AS, probably because
667 participants could make their perceptual judgment earlier in the AS Intervening task than the AT
668 Intervening task. In the auditory WM conditions, no significant clusters were found in the later
669 (3.5-5 sec) time window.

670 In the visual WM conditions without an Intervening task, alpha power gradually returned
671 from the suppression during WM encoding to near-baseline levels during WM retention (Fig. 6C,
672 top panel). On trials with an AS Intervening task, there was a tendency for alpha to become

673 suppressed again after the conclusion of the Intervening task (bottom panel). We examined these
674 alpha power time courses using cluster-based permutation testing restricted to the same time
675 windows as in the auditory WM conditions: 2 to 3.5 sec and 3.5 to 5 sec from the start of the WM
676 retention phase. Unlike the auditory conditions, no significant differences were observed during
677 the Intervening tasks. However, in the later window, when the Intervening task was AS, alpha
678 power was significantly reduced relative to when there was no Intervening task ($p = 0.011$; Fig.
679 6D). This alpha reduction did not reach significance following the AT Intervening task. When the
680 cluster formation threshold was again relaxed to $p < 0.05$, alpha power was found to be
681 significantly lower following the AS Intervening task than the AT task ($p = 0.027$, not shown). In
682 other words, the alpha suppression present during visual WM encoding resumed following the
683 spatial Intervening task, possibly representing a signature of domain-driven interference.

684 Finally, the presence of either Intervening task also caused an increase in frontal theta (4-
685 7 Hz) power throughout the memory retention window (Supplemental Fig. 4). In all but one of the
686 conditions with an Intervening task, cluster-based permutation tests revealed at least one time-
687 channel cluster in which theta power was significantly elevated relative to the corresponding no
688 Intervening task conditions ($p < 0.05$ for all clusters). In the remaining condition (AT WM, AS
689 Intervening task), a similar increase in theta power was trending toward significance ($p = 0.053$).
690 Although ERPs can manifest as activity in this frequency range as well, the increase in theta power
691 was observed both preceding and well after the Intervening task, meaning it cannot easily be
692 explained by evoked responses. Frontal-midline theta power and theta-band phase coupling in
693 fronto-parietal networks have been linked to task-switching (Cunillera et al., 2012; López et al.,
694 2019; Sauseng et al., 2006) and high levels of cognitive load (Gevins, 1997; McEvoy et al., 2000),
695 both of which were likely relevant in conditions with an Intervening task.

696 **Discussion**

697 We used a dual-task paradigm, comprising WM and auditory Intervening tasks, to investigate
698 processing interference as a function of whether the two tasks matched in sensory modality and
699 information domain. Convergent evidence from behavior and pupillometry showed that processing
700 was negatively impacted when the two tasks drew upon shared processing resources. Specifically,
701 this manifested as the highest Intervening task error rates, poorest memory retrieval, and largest
702 pupil dilations when both tasks were auditory-temporal. We expected auditory-temporal WM
703 information to load exclusively on auditory-biased attention and WM networks, likely increasing
704 interference with the auditory Intervening tasks. In contrast, auditory-spatial and visual WM
705 information was likely mapped to and maintained in visual-spatial networks, protecting it from
706 interference by the auditory Intervening tasks. Measures of interference were smallest in the visual
707 WM conditions, and they did not differ depending on whether the WM task was temporal or
708 spatial. This suggests that interference was minimal when competing tasks were presented in
709 different sensory modalities.

710 In these conditions with reduced competition for shared neural resources, subtler patterns
711 of dual-task interference were nonetheless revealed in the neural data. The amplitudes of the P2
712 components of auditory ERPs elicited by Intervening task onset tended to be suppressed by dual-
713 task similarity in either modality or domain. The largest P2 components were observed in visual
714 WM conditions when the information domain was mismatched between the two tasks. Ongoing
715 alpha (8-13 Hz) oscillations during WM maintenance were also modulated by the presence of an
716 Intervening task. In the auditory WM conditions, alpha power was strongly interrupted by both the
717 AT and the AS Intervening tasks. In the visual WM conditions, alpha power was suppressed
718 following selectively the auditory-spatial Intervening task, possibly indicating the need to re-

719 engage WM mechanisms more strongly after interruption of visual WM rehearsal by spatial
720 processing in a different sensory modality.

721

722 *Similarity in sensory modality leads to increased dual-task interference*

723 While this is the first study we are aware of to investigate how both sensory modality and
724 information domain influence dual-task interference, several previous behavioral studies have
725 determined that interference depends on some axis of similarity between two simultaneous tasks.
726 For instance, Kim et al. (2005) reported increased Stroop task interference when WM was loaded
727 with verbal information that overlapped with the Stroop target. On the other hand, there was no
728 effect of loading WM with spatial information irrelevant to the Stroop task, and loading WM with
729 information similar to the Stroop task distractor actually reduced interference. Similarly, when
730 participants have to retrieve both the orientation and location of visual items, visual distractors that
731 differ from the target only in orientation selectively impair retrieval of target orientation, but not
732 location (Marini et al., 2017). In the realm of phonological WM, distractor words presented during
733 WM retention selectively interfere with recall of words with which they share phonological
734 properties (Oberauer & Lange, 2008).

735 In line with the current study, previous work has specifically implicated similarity in
736 sensory modality as a determinant of distractor and dual-task interference. For instance, auditory
737 and visual discrimination thresholds (for pitch and contrast, respectively) are unaffected by
738 concurrent, irrelevant stimuli in the opposite modality, but are considerably higher in the presence
739 of concurrent stimuli in the same modality (Alais et al., 2006). In dual-task paradigms, increased
740 interference has been observed when both tasks are tactile, auditory, or visual, as compared to
741 conditions in which the tasks were presented in different modalities (Morrison et al., 2015; Scerra

742 & Brill, 2012). These results lend support to multiple resource theory, which states that
743 interference between two tasks depends on whether they compete for the same set of limited neural
744 resources.

745

746 *Dual-task interference: A single central or task-specific bottleneck?*

747 The neural underpinnings of dual-task interference have been the topic of substantial debate. An
748 opposing view to the multiple resource theory posits that a general, “central bottleneck” limits
749 performance independently of the specific processing demands of the component tasks (Pashler,
750 1998); a number of neuroimaging studies have provided support for this view (Dux et al., 2006;
751 Marois & Ivanoff, 2005; Tombu et al., 2011). However, contrasting studies more in line with
752 multiple resource theory have shown that interference is marked by increased activity in the brain
753 regions involved in processing the component tasks, without recruitment of any additional areas
754 in dual-task conditions (Adcock et al., 2000; Bunge et al., 2000). This has also been observed at
755 the level of single neurons, with dual-task interference being linked to reduced representational
756 fidelity in a shared population of lateral prefrontal cortex neurons required for both tasks
757 (Watanabe & Funahashi, 2014).

758 In the current study, we attempted to differentially load auditory- and visual-biased
759 cortical networks with our dual-task paradigm. Recruitment of these two networks for attention
760 and WM processing is clearly differentiable based on both sensory modality and information
761 domain (Michalka et al., 2015, 2016; Noyce et al., 2017), supporting the view that they are
762 physiologically distinct neural resources. On the other hand, each network is recruited by a variety
763 of tasks within its preferred modality and domain. Thus, two related but unidentical tasks could
764 interfere with each other if they both load onto the same cortical network, consistent with a “central

765 bottleneck.” The coexistence of these properties suggests that the central bottleneck and multiple
766 resource accounts of dual-task interference may not be entirely dichotomous, an idea supported by
767 the present results. Interference patterns measured with behavior and pupillometry were generally
768 similar between the AT and AS Intervening tasks, indicating that both Intervening tasks loaded
769 predominantly onto the same network (likely the auditory-temporal network), despite one
770 involving temporal processing and the other spatial processing (i.e., an apparent central
771 bottleneck). In the WM task on the other hand, dual-task interference patterns were strikingly
772 different between the AT and AS WM conditions. The AS WM task required participants to map
773 absolute sound locations into exocentric coordinates, which likely drove the visual-spatial network
774 more than the AS Intervening task, which only required an immediate comparison of two sets of
775 interaural cues. In other words, the AS WM task was likely able to recruit a separate pool of neural
776 resources, reducing interference from the auditory Intervening tasks; this result is more consistent
777 with multiple resource theory. Thus, there may not be a clear and generalizable resolution between
778 these two theories; rather, dual-task interference effects likely depend on relationships between the
779 specific tasks used, and the specific brain regions and networks these tasks recruit.

780 Another noteworthy aspect of the results presented here is that the processing costs of
781 loading onto a single network (measured as increased behavioral interference, larger pupil
782 diameter, and ERP amplitude suppression) were greater than the costs of switching between
783 networks. This outcome is not entirely obvious, as task-switching also incurs a processing cost
784 (Arnell & Jolicœur, 1999; Chun & Potter, 2001; Hsieh & Allport, 1994; Meiran et al., 2000). Our
785 auditory Intervening tasks did modestly impair visual WM retrieval, consistent with a behavioral
786 cost of switching between the complementary networks. However, this effect was relatively weak
787 compared to the behavioral (and physiological) costs when the tasks loaded onto shared network

788 resources. Thus, the ability to simultaneously leverage complementary attention and WM networks
789 appears to confer a processing benefit, which may be especially relevant in complex, multisensory,
790 real-world environments.

791

792 *Separate contributions of behavioral, pupillometry, and EEG measures*

793 Measures of behavior, pupillometry, and EEG in this study each offered unique insights into the
794 dual-task interference at play. Pupillometry was included because it can serve as a sensitive
795 biomarker of the cognitive effort required to achieve a certain performance level, even in the
796 absence of behavioral differences. For instance, maximum pupil dilations evoked by speech are
797 larger for listeners with hearing loss than normal-hearing controls, even when the signal-to-noise
798 ratio is high enough for both groups to achieve ceiling performance. This is thought to reflect a
799 heightened degree of listening effort, not captured by behavioral measures alone (Ohlenforst et al.,
800 2017). Pupil dilations have also been shown to correlate with participants' subjective assessments
801 of task difficulty (Koelewijn et al., 2015). In the present study, this benefit manifested in our ability
802 to detect differences between the AT and AS WM conditions when the Intervening task was AS.
803 This Intervening task was easy enough that a majority of participants did not make errors on it in
804 any WM condition. However, substantial differences in the amplitude of pupil dilations elicited
805 by the AS Intervening task indicated that the information in WM did cause processing interference,
806 which participants overcame to achieve excellent performance.

807 In addition, behavioral performance on each trial is often a single-sample snapshot,
808 encompassing all the processing dynamics present in the task. Pupillometry allows for more fine-
809 grained dissection of the time course of these dynamics. For instance, pupil data in this study
810 revealed that participants were modulating their effort level to encode AT information in WM

811 when an auditory Intervening task would be present, indicating preparation for a challenging
812 interference condition. Analysis of the temporal dynamics of pupil responses is becoming more
813 common in other fields as well, including the study of cognitive processes that unfold through time
814 like decision making (Satterthwaite et al., 2007) and the perception of temporally complex inputs
815 like speech and music (Jagiello et al., 2019; Winn & Moore, 2018). Conversely, though, the
816 behavioral data provided insights that would have been difficult to glean from pupillometry alone.
817 Pupil responses elicited by the Intervening task stimuli were drastically different from the no
818 Intervening task conditions, making it difficult to interpret the magnitude of the interference
819 effects. The behavioral data puts this in more concrete terms; we could measure exactly how much
820 performance on each task was influenced by the other. Because of these complementary benefits,
821 we argue that pupillometry data are best interpreted alongside corresponding behavioral measures.

822 In the visual WM conditions, interference by the auditory Intervening tasks was generally
823 low, and neither behavioral nor pupil responses differed based on whether the information held in
824 WM was temporal or spatial. This finding was counter to our expectations; for instance, we
825 expected to observe mild interference when the Intervening and WM tasks were both spatial.
826 Auditory and visual spatial processing are known to be represented in the EEG response, often in
827 the form of lateralized alpha oscillations at parietal scalp locations (Bednar & Lalor, 2018; Deng
828 et al., 2020; Kelly et al., 2006; Klatt et al., 2018; Thut et al., 2006; Tune et al., 2018; Worden et
829 al., 2000). Given the sensitivity of EEG to spatial processing, we expected to observe domain-
830 based interference patterns in our EEG data when the WM and Intervening tasks were both spatial.
831 Indeed, ERPs and alpha modulations proved particularly sensitive to these subtle interference
832 patterns, which did not affect error rates or pupil responses. The P2 components of ERPs were
833 largest when the tasks were presented in different modalities and, in the case of the visual WM

834 conditions, when the information domains of the tasks were also mismatched. This pattern is
835 consistent with greater availability of processing resources when the tasks did not compete for
836 shared modality- and domain-biased neural resources (Kok, 1997).

837 We found that alpha power was modulated by the presence of an Intervening task and by
838 its information domain. This alpha had a more anterior and centralized distribution than the
839 lateralized alpha often implicated in spatial attention (Fig. 6). Alpha power with the scalp
840 distribution we found in this study has been linked to various types of WM load, including visually
841 presented letters and numbers (Jensen et al., 2002; Klimesch et al., 1999; Schack & Klimesch,
842 2002), shape information (Herrmann et al., 2004; Johnson et al., 2011), spatial information
843 (Bastiaansen et al., 2002), and auditory stimuli (Lim et al., 2015; Obleser et al., 2012; Vogt et al.,
844 1998). In the auditory WM conditions, the auditory Intervening tasks interrupted this alpha activity
845 during WM retention. This is consistent with previous work showing that distracting visual stimuli
846 interrupt alpha power during retention of both auditory and visual information in WM (Hakim et
847 al., 2020; Mishra et al., 2013). In the visual WM conditions, alpha power was suppressed relative
848 to baseline during WM encoding, perhaps due to the need to attend task-relevant visual stimuli
849 (Foxe & Snyder, 2011; Jensen & Mazaheri, 2010). In these conditions, there was no significant
850 change in alpha power during Intervening task presentation; however, following the spatial
851 Intervening task, the alpha suppression resumed. The functional implications of these alpha
852 suppressive effects, and why their pattern differed between the auditory and visual WM conditions,
853 are topics warranting targeted future investigation.

854

855 **Conclusions and future directions**

856 In a dual-task paradigm designed to drive auditory- and visual-biased attention and WM networks,
857 we reported behavioral, autonomic, and electrophysiological signatures of interference when the
858 tasks drew upon shared neural control resources. Future studies should implement a similar
859 paradigm with fMRI to pinpoint the neural networks involved in this kind of dual-task interference,
860 as well as invert the paradigm used here – using visual rather than auditory Intervening tasks – to
861 test whether interference patterns flip under opposite network demands.

862

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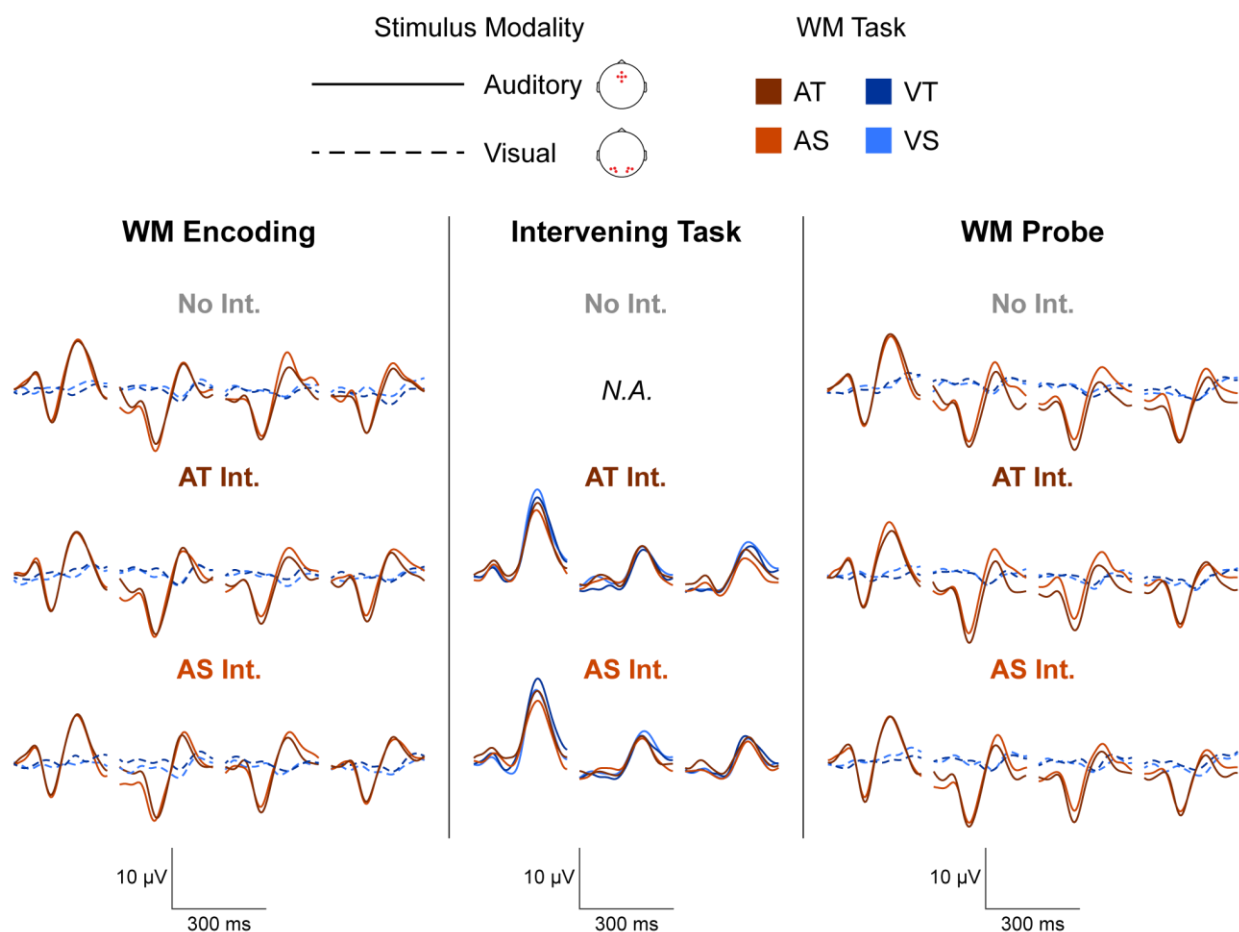
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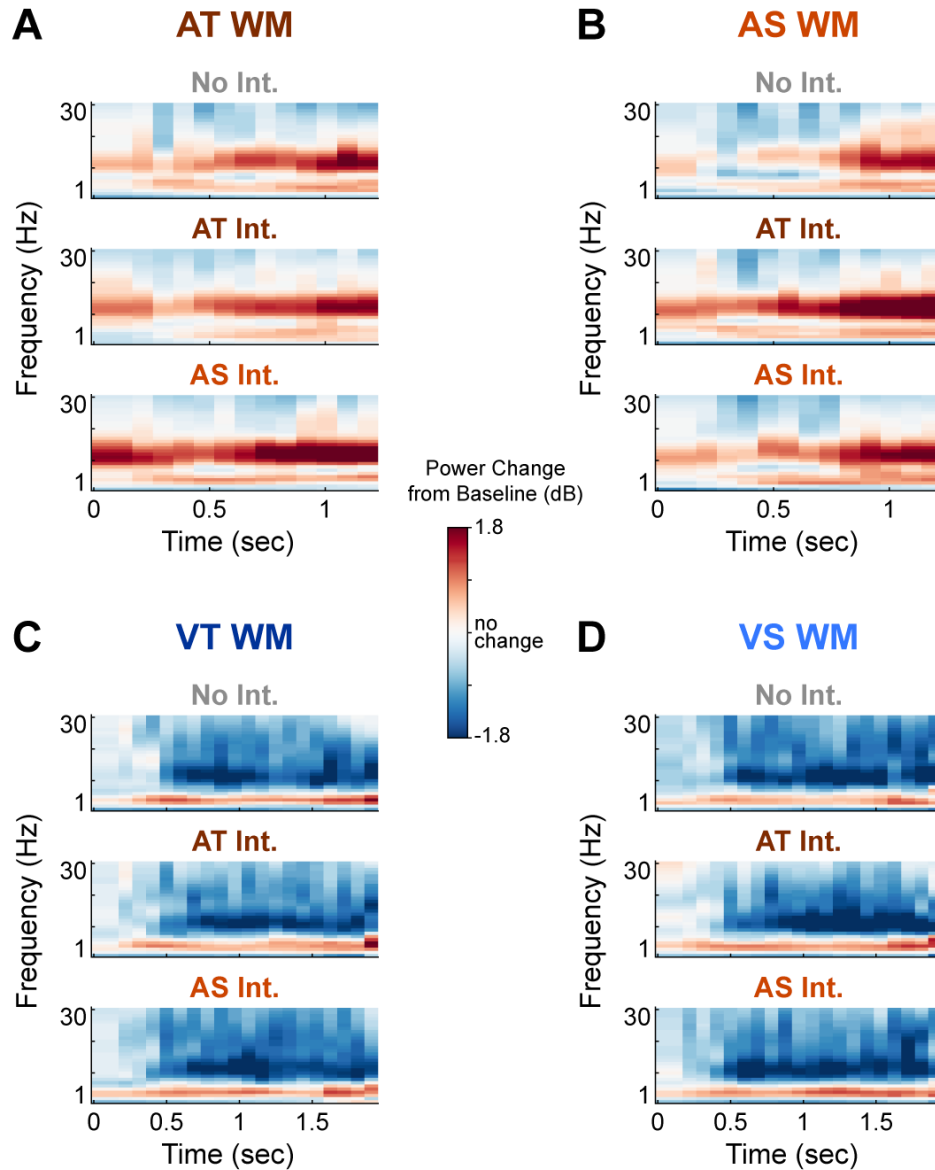
1163 **Supplemental Figures**



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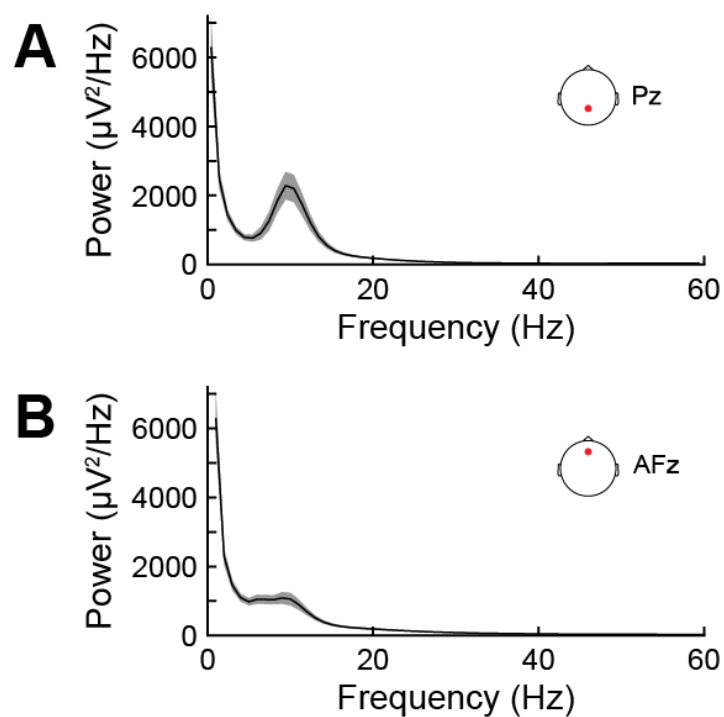
1165 **Supplemental Figure 1: Grand average ERPs for each combination of WM task (colors), Intervening**
1166 **task (rows), and position in the stimulus sequence.** The modality of stimulus presentation is shown by
1167 solid versus dashed lines. The top-left legend shows the channels averaged to produce ERPs for each
1168 stimulus modality: on the standard 10-20 layout, these were channels Fz, AFz, Cz, F1, and F2 for auditory
1169 stimuli and O1, O2, PO3, PO4, PO7, PO8 for visual stimuli. Axes below the data in each trial phase are
1170 shown for scale.

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1173 **Supplemental Figure 2:** Grand average oscillatory power during WM encoding in the AT (A), AS (B),
1174 VT (C), and VS (D) WM conditions. Data are shown as change relative to the pre-trial baseline, in dB.
1175 Alpha power strengthened relative to baseline during auditory WM encoding and became suppressed
1176 relative to baseline during visual WM encoding. Because the length of the encoding window differed based
1177 on inter-stimulus intervals, responses of different lengths were aligned to the end of the encoding phase
1178 prior to averaging. Similarly, because the long interval was longer for visual WM than auditory WM, the
1179 time bases differ between the top and bottom panels.
1180



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1182 **Supplemental Figure 3:** Grand average power spectra during the pre-trial baseline, plotted separately at
1183 channel Pz (A) and channel AFz (B). Note the well-defined peak in the alpha (8-13 Hz) frequency range at
1184 the parietal electrode site. Theta (4-7 Hz) power was more task-induced and so was less strong during
1185 baseline at the frontal electrode site; nonetheless, the power spectrum in panel B flattens around this
1186 frequency range at a higher value than at the parietal electrode site. Error clouds represent S.E.M.

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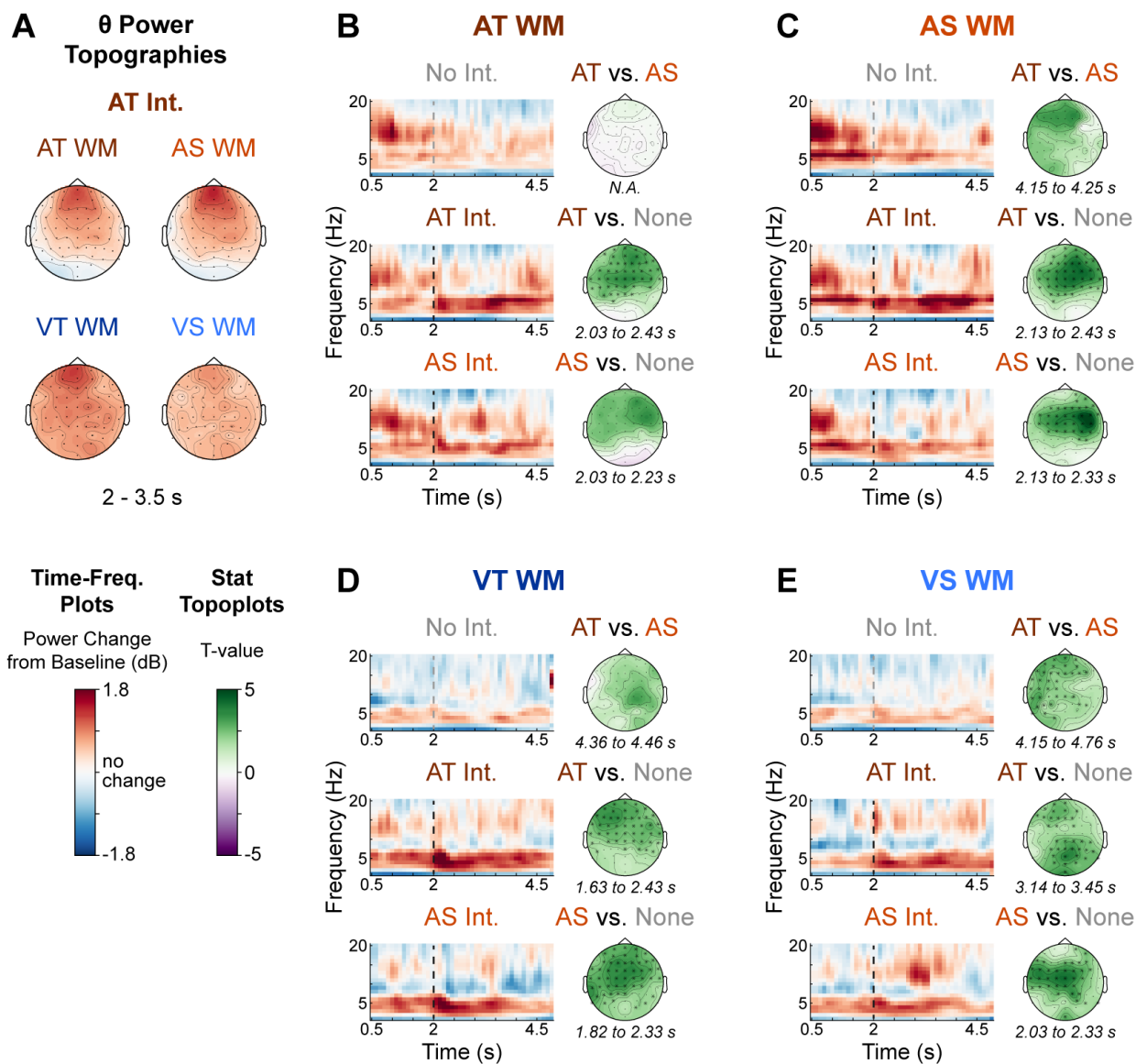
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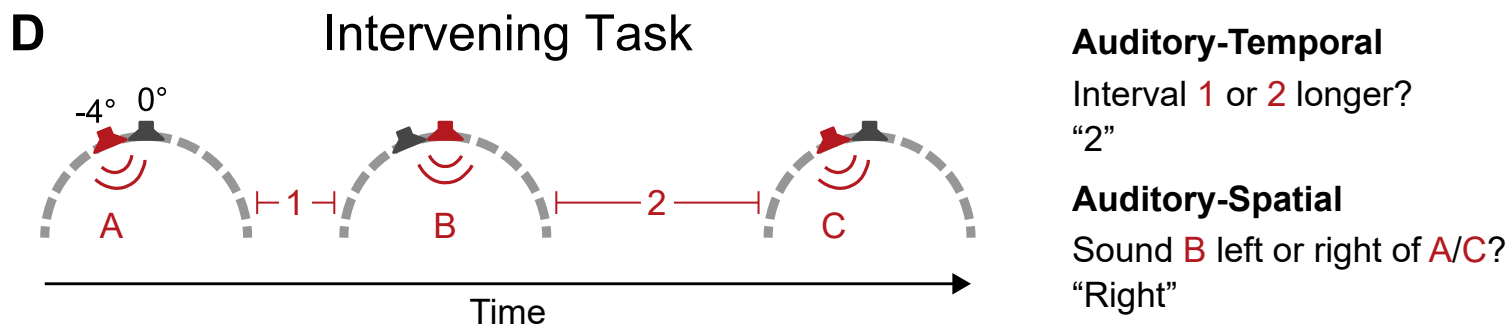
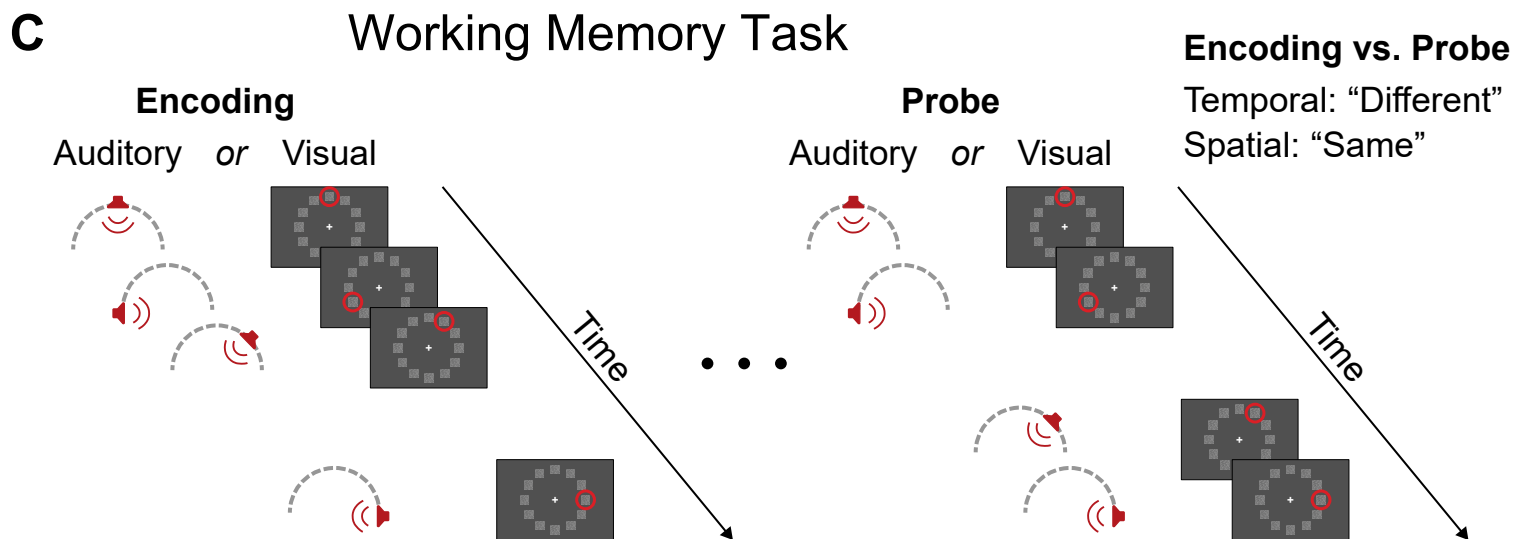
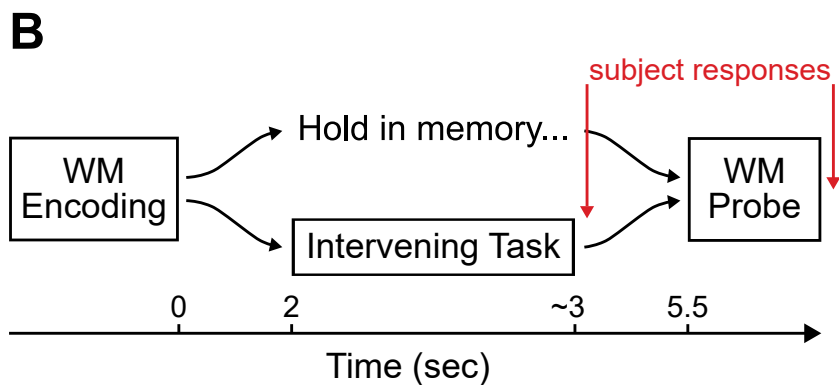
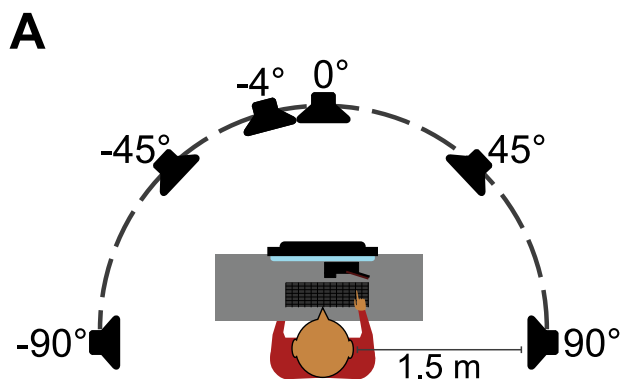
θ -Band (4-7 Hz) Activity

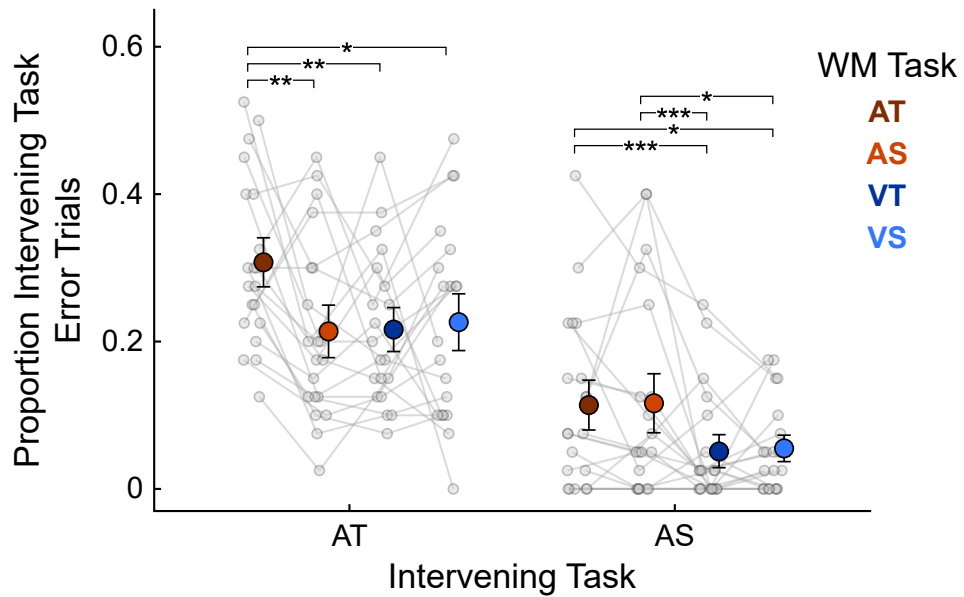


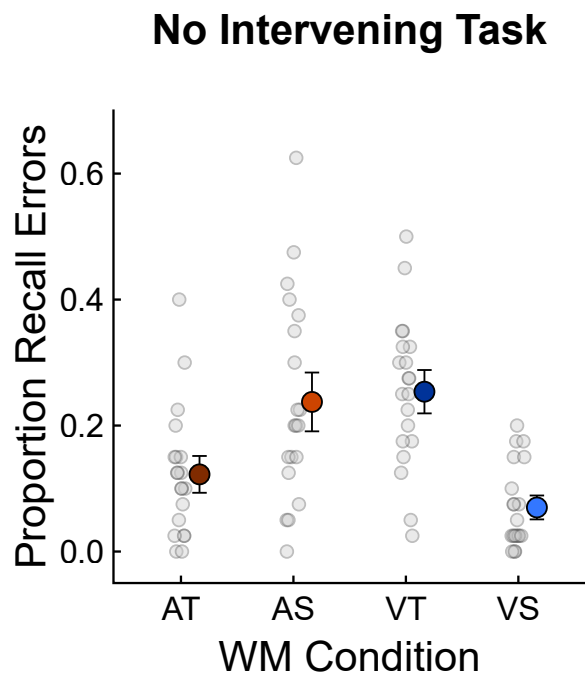
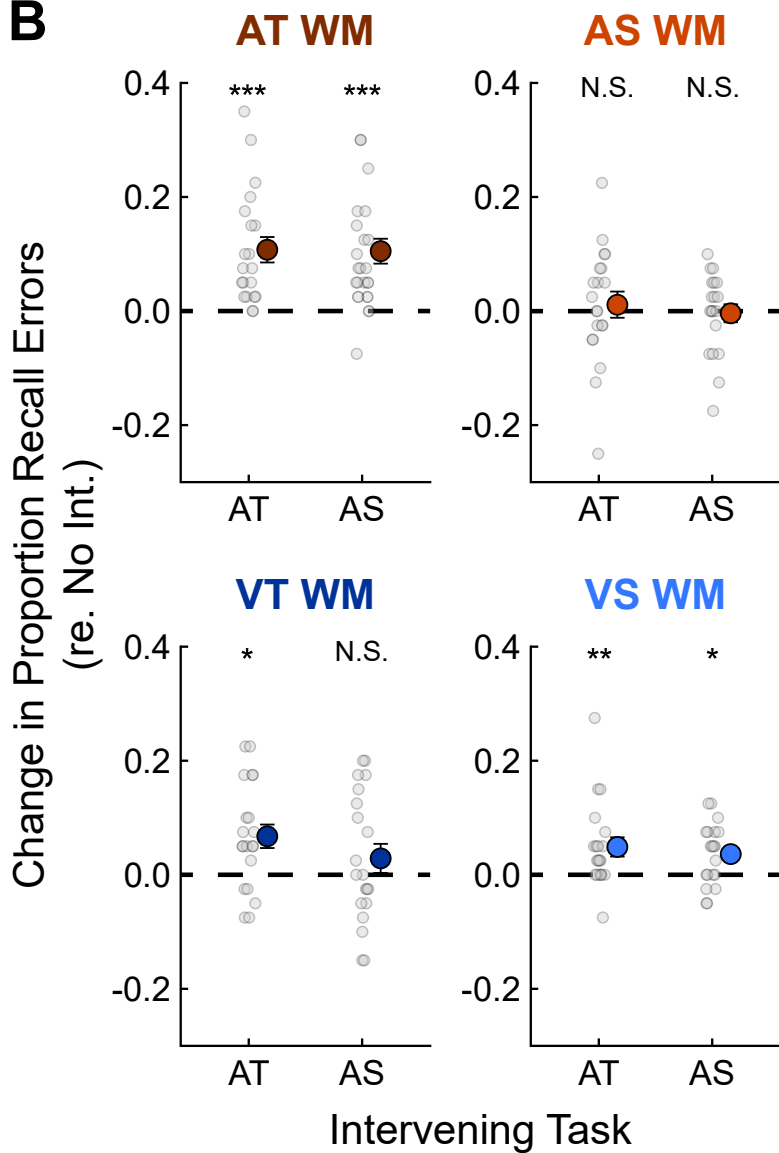
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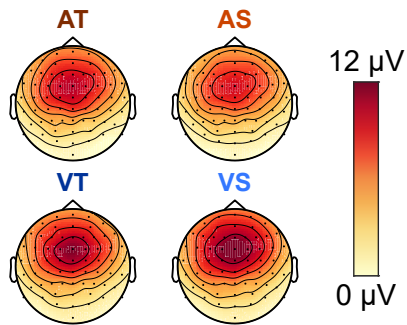
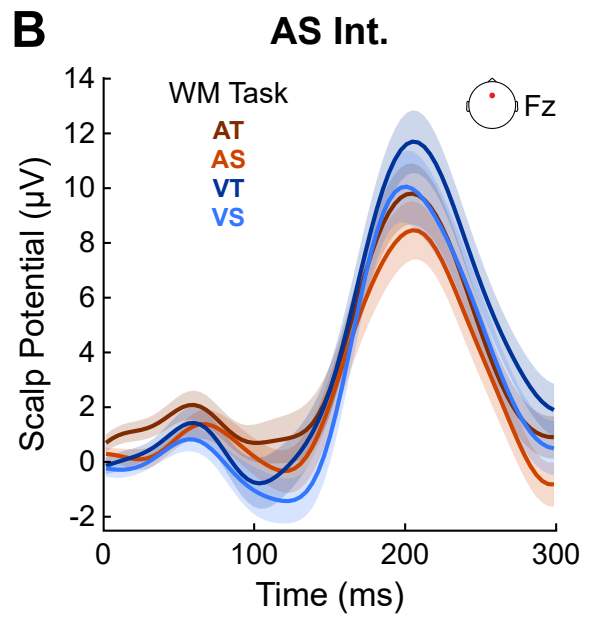
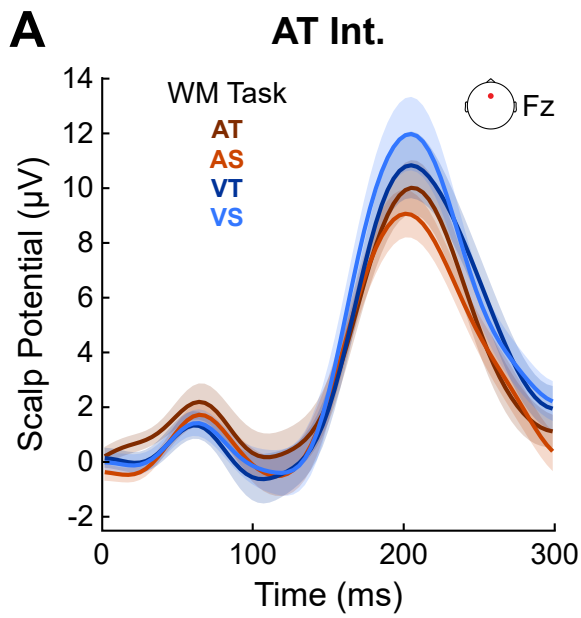
1197 **Supplemental Figure 4: Increased theta (4-7 Hz) power in conditions with an Intervening task. A,**
 1198 Topographies of theta power when the Intervening task was AT, shown to illustrate the fronto-central
 1199 concentration of theta power. **B-E**, Left panels show time-frequency responses at a fronto-central
 1200 electrode site (AFz) relative to the pre-trial baseline. Within each WM task, scalp topographies to the
 1201 right show the results of cluster-based permutation tests comparing the indicated Intervening task
 1202 conditions. T-values from cluster formation are plotted on the green-purple axis, as in some cases, outlier
 1203 participants with Supplemental Figure 3.12 (Continued): anomalously strong theta power changes
 1204 exaggerated the apparent differences in the grand average time-frequency plots. Asterisks signify
 1205 membership in a significant cluster ($p < 0.05$). For each comparison, only the strongest time-channel
 1206 cluster is shown, although some comparisons did yield multiple significant clusters. If the strongest
 1207 cluster identified did not reach significance, the topoplot is nonetheless restricted to the time region of

1208 that cluster. If no clusters were identified, the topoplot time range spans the entire WM retention window
1209 (time shown as N.A.).

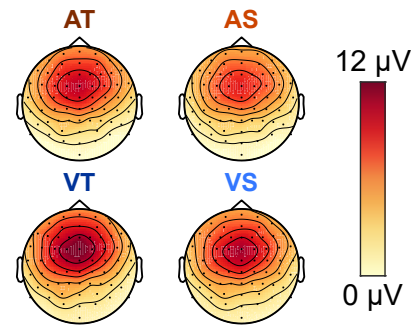




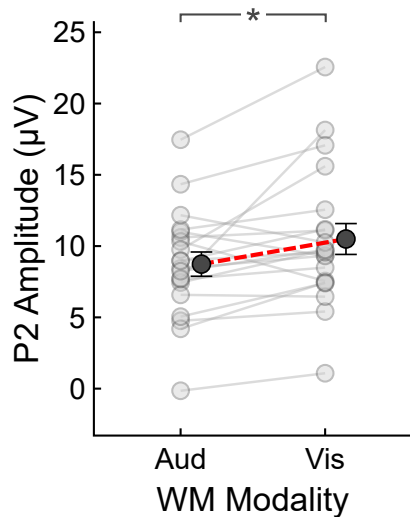
A**B**



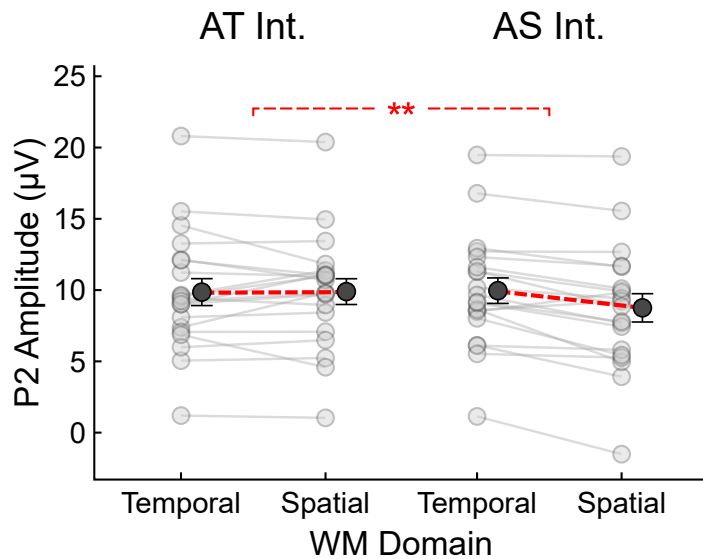
*P2 topographies
(190-220 ms)*



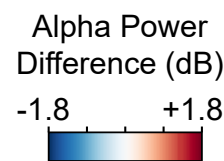
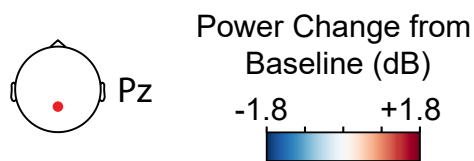
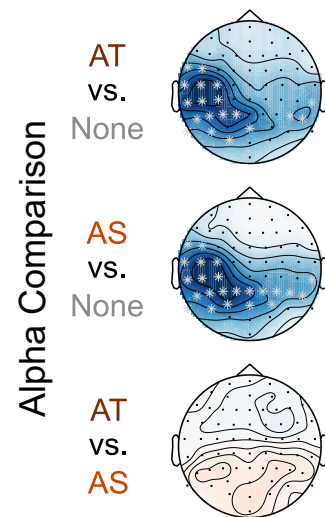
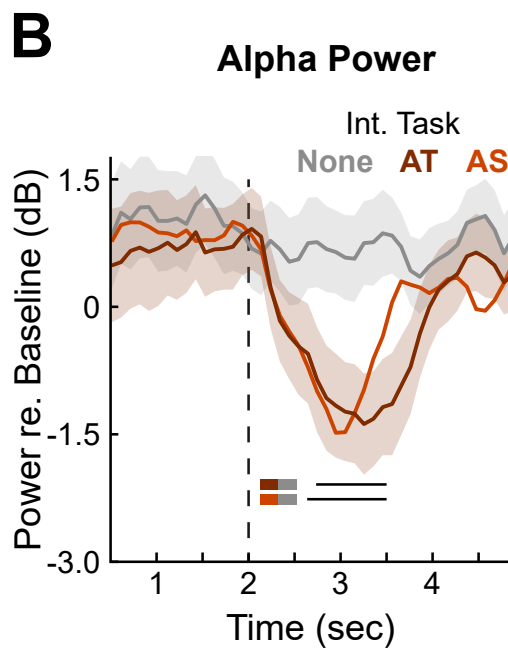
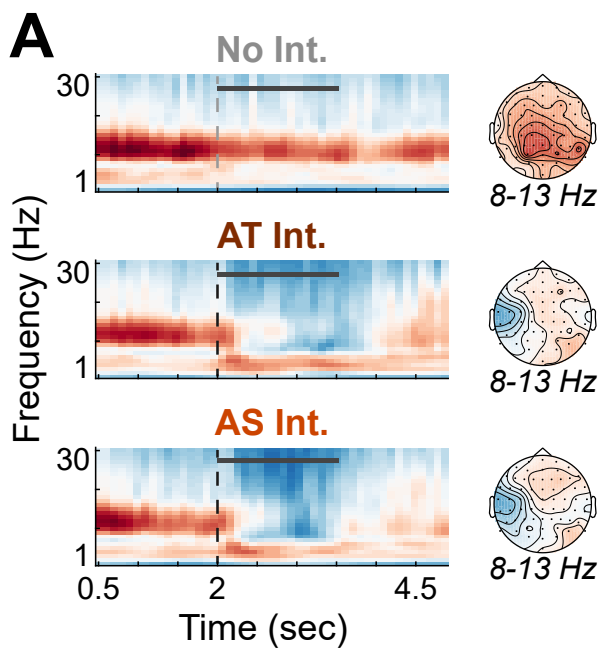
C Modality Main Effect



D Domain – Int. Task Interaction



Auditory WM



Visual WM

