Fluorinated oil-surfactant mixtures with the density of water: artificial cells for synthetic

biology

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Abstract

There is a rising interest in biotechnology for the compartmentalization of biochemical

reactions in water droplets. Several applications, such as the widely used digital PCR,

seek to encapsulate a single molecule in a droplet to be amplified. Directed evolution,

another technology with growing popularity, seeks to replicate what happens in nature

by encapsulating a single gene and the protein encoded by this gene, linking genotype

with phenotype. Compartmentalizing reactions in droplets also allows the

experimentalist to run millions of different reactions in parallel. Compartmentalization

requires a fluid that is immiscible with water and a surfactant to stabilize the droplets.

While there are fluids and surfactants on the market that have been used to accomplish

encapsulation, there are reported concerns with these. Span® 80, for example, a

commonly used surfactant, has contaminants that interfere with various biochemical

reactions. Similarly, synthetic fluids distributed by the cosmetic industry allow some

researchers to produce experimental results that can be published, but then other

researchers fail to reproduce some of these protocols due to the unreliable nature of

these products, which are not manufactured with the intent of being used in

biotechnology. The most reliable fluids, immiscible with water and suitable for

biochemical reactions, are fluorinated fluids. Fluorinated compounds have the peculiar

characteristic of being immiscible with water while at the same time not mixing with

hydrophobic molecules. This peculiar characteristic has made fluorinated fluids

attractive because it seems to be the basis of their being biologically inert. However,

commercially available fluorinated fluids have densities between 1.4 to 1.6 g/mL. The

higher-than-water density of fluorinated oils complicates handling of the droplets since

these would float on the fluid since the water droplets would be less dense. This can

cause aggregation and coalescence of the droplets. Here, we report the synthesis,

characterization, and use of fluorinated polysiloxane oils that have densities similar to

the one of water at room temperature, and when mixed with non-ionic fluorinated

surfactants, can produce droplets encapsulating biochemical reactions. We show how

droplets in these emulsions can host many biological processes, including PCR, DNA

origami, rolling circle amplification (RCA), and Taqman® assays. Some of these use

unnatural DNA built from an Artificially Expanded Genetic Information System (AEGIS)

with six nucleotide "letters".

Introduction

There is a growing interest in the biochemical sciences for the compartmentalization

or miniaturization of reactions [1] [2]. When conducted in water-in-oil droplets,

compartmentalization allows experimentalists to run millions of reactions in parallel,

creating ample opportunity to analyze the vast diversity contained within a biochemical

sample. One can amplify an isolated gene in a digital PCR or explore the vast protein

sequence space in directed evolution experiments [3]. Approaches such as directed

evolution and/or high throughput screening require sequence diversity. These kinds of

experiments require to isolate variants of a biomolecule. In some cases, enzymes can

be isolated with their encoding genes and can be, considered by some, as forming a

sort of "artificial cell". One way to achieve this compartmentalization and screening is

with the use of water-in-oil droplets [4]. These "artificial cells" [5] [6] and other

compartments have several applications, including drug delivery [7-9], enzyme directed

evolution [10, 11] [12, 13] [1] [14], and models for the origin of life [15-19]. While water-

hydrophobe-water systems are analogs of natural cells [20] [21] [22-25], simple water-

in-oil emulsions are intrinsically easier to assemble and more stable to environmental

change (especially heating) as compartment analogs of cells.

As with standard cells, compartments can maintain a link between the structures of

molecules inside the droplet (the "phenotype") and the structures of the molecules that

encode them (the "genotype"). This is important when experimentalists seek to direct

the evolution of nucleic acids and their encoded proteins under selective pressure. For

example, compartmentalization in two-phase artificial cell systems has been used for

directed evolution [3] in the form of "compartmentalized self replication" (CSR).

Developed by Tawfik and Griffiths, CSR holds proteins and genes together in water

droplets suspended in oil emulsions [26]. CSR was applied to the directed evolution of

DNA polymerases by Holliger and his collaborators [10]. CSR has also been used to

select DNA polymerases that accept unnatural nucleotides [12] [27].

Compartmentalization is of great interest to synthetic biologists, who seek to put alien

"xeno" nucleic acids (xNAs) into artificial cells. One example of xNA are artificially

expanded genetic information systems (AEGIS) that increase the number of

independently replicable nucleotides from 4 to as many as 12 [28] . By shuffling

hydrogen bonding patterns of the G:C and A:T pairs while retaining their Watson-Crick

size-complementarity [28]. AEGIS DNA can evolve to produce aptamers molecules that

bind to liver and breast cancer cells [29] and isolated proteins [30]. Modified nucleic

acids can potentially be used as therapeutics [31]; recently some AEGIS components

have been suggested as potential inhibitors of the RNA polymerase from SARS-CoV-2

[32]. The Z:P pair from AEGIS used in this work is shown in Fig 1.

Figure 1. The Z:P pair from an Artificially Expanded Genetic Information System

(AEGIS), left. AEGIS nucleotides follow the geometry and hydrogen bonding

architecture of the natural nucleotides. The hydrogen bonding patterns are named pu or

py, depending on whether they are presented on a large (purine-like) or small

(pyrimidine-like) heterocyclic ring system respectively. Hydrogen bond donor (D) and

acceptor (A) groups listed starting in the major groove and ending in the minor groove.

Unshared pairs of electrons presented to the minor groove are shown in green orbitals.

The Z:P pair presents the pyDDA:puAAD hydrogen bonding pattern, while the analog

C:G pair presents the pyDAA:puADD. R is deoxyribose.

Compartmentalization in water-in-oil droplets requires a fluid immiscible with water

and a surfactant. The surfactant must lower the surface tension of the liquid, stabilize

the emulsion, and diminish coalescence [33] [34]. There are several commercially

available surfactants and fluids for this purpose; however, there are some difficulties

with these. For instance, in our laboratory, Span® 80 has been used to produce water-

in-oil droplets, but we have known for years that there are observable differences

between batches of the same product (S1 Fig.) potentially arising from the fact that it is

derived from animal fat. In our experience, directed evolution experiments using

Span80® proved unreliable. We have observed dark precipitates at the bottom of bottles

of Span80® and in oil phases with Span80®-based mixtures (S2 Fig.). Furthermore, the

same authors who pioneered the use of Span® 80 for creating water-in-oil droplets

have reported the presence of contamination with peroxides [35] [36], which interferes

with some biochemical processes. To counter these issues, silicone fluids were

proposed as an alternative. There are many examples of research done with silicone

fluids that come from the cosmetic industry. Some, commercialized by Degussa (now

Evonik), are not available commercially in research-sized amounts. One cannot expect

that a batch of a silicone fluid to be used for producing sunscreen would go through

testing for its suitability for PCR. For example Diehl *et al.* report the use of ABIL WE09

from Degussa for water-in-oil emulsions but notes in the supplementary section that

dark precipitates are observed [37]. Not surprisingly some researchers fail to replicate

the protocols published by other groups or at least need to modify some of the protocols

[1]. The lack of more choices of surfactants for biotechnology have motivated other

researchers to create their own biocompatible surfactants as well [38].

There are several commercially available fluorinated fluids, which are used for

microfluidics. Fluorinated fluids have peculiar properties; they are immiscible with water

and hydrocarbons, forming a third "flourous" phase. As natural proteins, membranes,

and other biomolecular systems exploit both hydrophilic and hydrophobic phases, a

purely hydrophobic oil or surfactant can disrupt biological systems because the

hydrophobic portion of the surfactants can invade the hydrophobic cores of proteins and

other biologics, disrupting their function. The fluorous phase comprising fluorinated

species is sufficiently "orthogonal" to both hydrophilic and hydrophobic systems as to

render that third phase inert with respect to most biological molecules systems

containing them. Thus, fluorinated oils are used for drug delivery [39, 40], blood

substitutes [41, 42], and diagnostics [43]. Several fluorinated oils and surfactants are

now commercially available for water-in-oil emulsions, and several of these are widely

used. These, however, have densities considerably higher than water, so the water

droplets float, which makes it difficult to manipulate them for instance for re-injection.

For example, the fluorinated oil HFE-7500 has a density of ~ 1.6 g/mL [44] [45].

Fluorinert[®] FC40 has a density between 1.845 and 1.895 [46] [47] [48]. Concentration of

the droplets in the top of the fluid also increases the number of droplet-droplet

encounters, which encourages droplet fusion.

These considerations provided the motivation to seek fluorinated oils that have a

density close to 1 g/mL, the density of aqueous solutions in which biological processes

act. The synthesis of silicones from hexamethylcyclotrisiloxane by ring-opening

polymerization has been reported before [49]. We report here the synthesis,

characterization of polysiloxanes, prepared by ring-opening polymerization under

conditions that produce fluids with densities near 1 g/mL while having enough

fluorinated monomers to be able to dissolve non-ionic fluorinated surfactants that

enable their use for the encapsulation of biochemical reactions.

Materials and methods

Materials

Hexamethylcyclotrisiloxane, 1,3,5-trimethyl 1,3,5-tris(3,3,3 trifluoropropyl)

cyclotrisiloxane, and 2,4,6,8-tetramethylcyclotetrasiloxane were purchased from

Changzhou Fluoride Chemical Co. Genuine Technology. Hexamethyldisiloxane was

purchased from Acros. Amberlyst® 15 hydrogen form and potassium trichloro(ethylene)

platinate (II) hydrate were purchased from Sigma-Aldrich.

Nonafluorohexyldimethylchlorosilane, 3,3,3 trifluoropropyldimethylchlorosilane;

allyloxy(polyethylene oxide) (4-7 EO); allyloxy(polyethylene oxide), methyl ether (6-8

EO) were obtained from Gelest. All chemicals were used without purification. Oligos

containing artificial nucleotides, artificial triphosphates dZTP, dPTP were obtained from

Firebird Molecular Biosciences. Phi29 polymerase and Exonuclease I were purchased

from New England Biolabs. CircLigase™ was purchased from Lucigen. Snap-Cap

Microcentrifuge Biopur™ Safe-Lock™ or Safe-Lock Tubes 2 mL were from

Eppendorf™. Stainless steel balls, 6 mm were obtained from IKA. EvaGreen® Dye 20X

in water was from Biotium. For DNA origami: a "Folding kit basic p7249 Cuboid with

large aperture" was obtained from Tilibit Nanosystems. All natural DNA oligos and

fluorescent probes were obtained from IDT.

Ring-opening polymerization

Polysiloxanes were prepared by the ring-opening reaction shown on Fig 2. Two

different protocols were developed:

Protocol 1. The fluorinated monomer 1,3,5-trimethyl 1,3,5-tris-(3,3,3-trifluoropropyl)-

cyclotrisiloxane (12 g; 25.6 mmol) was mixed with the non-fluorinated monomer

hexamethylcyclotrisiloxane (72 g; 323.7 mmol) and hexamethyl disiloxane (3 mL; 14.1

mmol); the second acted as a chain terminator. The mixture was heated to 75 °C in an

oil bath. Amberlyst® 15 catalyst (1.2 g) was added once the reaction mixture was

homogeneous. The reaction proceeded under argon for 3 hours at 75 °C. Once cooled,

the reaction mixture was decanted from the solid Amberlyst® catalyst.

The products were then resolved by distillation under reduced pressure (23 mm Hg).

Unreacted materials were removed at 90 ºC while collecting a fraction of the fluorinated

fluid. After removing materials at 90 °C; the remaining fluid was labeled as Fluid A.

From this fluid a low molecular weight (LMW, Fluid B) fraction was obtained by

distillation (150 °C, 23 mm Hg); a high molecular weight fraction remained, non-distilled

(HMW fraction).

Protocol 2. The fluorinated monomer 1,3,5 trimethyl 1,3,5-tris(3,3,3-trifluoropropyl)

cyclotrisiloxane (25.26 g; 53.9 mmol) was mixed with the non-fluorinated monomer,

hexamethylcyclotrisiloxane (36 g; 161.8 mmol) and hexamethyl disiloxane (2.8 mL;

13.11 mmol). The mixture was heated to 75 °C in an oil bath. Catalyst Amberlyst® 15

(1.2 g) was added last, again after the mixture was homogeneous. The reaction

proceeded under argon for 4 hours at 75 °C. Then, an opaque liquid was decanted to

separate it from the solid catalyst. Distillation using a Kugelrohr apparatus (90 °C, 23

mm Hg) removed unreacted starting materials. This remaining fluid was left at room

temperature for 8 hours, after which it had separated into two layers each with different

characteristics (top layer: fluid C; bottom layer: fluid D).

Figure 2. Ring-opening polymerization used to produce the fluorosilicone fluid.

The two cyclotrisiloxane monomers (hexamethylcyclotrisiloxane and 1,3,5-trimenthyl

1,3,5-tris(3,3,3-trifluoropropyl)cyclotrisiloxane) are reacted along with hexamethyl

disiloxane, which acts as a chain terminator. The catalyst Amberlyst® 15 acts as an

acid catalyst for the ring-opening reaction.

Fluorinated surfactants

Fluorinated hydrophilic chains were synthesized following the work of Kobayashi and

Owen [50]. Two fluorinated hydrophobes have been explored: 3,3,3-trifluoropropyl (Pr_f)

and 3,3,4,4,5,5,6,6,6-nonafluorohexyl (Hx_f). These hydrophobes were combined with

allyloxy(polyethylene oxide) following reference [50] with some modifications. The

surfactants (Fig 3) were prepared by hydrolysis of their chlorosilane precursors and

eventually bound to the hydrophile by hydrosilation with allyloxy(polyethylene oxide). A

scheme of the synthesis and details are provided in the supplementary information

section (S3 Fig.).

Figure 3. Nonionic fluorosilicone surfactants. The amphiphilic molecules are

produced by reacting SiH functionalized branched disiloxanes hydrophobes with

allyloxy(polyethylene oxide) following reference [50]. Two different hydrophiles (a, b)

and two hydrophobes are shown: one with the 3,3,3-trifluoropropyl (R_1, Pr_f) and

3,3,4,4,5,5,6,6,6-nonafluorohexyl (R_2, Hx_f).

Gel permeation chromatography

Gel permeation chromatography (GPC) was performed by Cambridge Polymer Group

(Boston, MA) using an Agilent 1100 Series HPLC Gel Permeation Chromatogram

equipped with an autosampler, thermostatted column oven, and refractive index

detector. The column used for the separation was the Agilent PLgel Mixed-B column (10

μm particle size; 300 mm X 7.5 mm) which has a nominal linear molecular weight

separation range from 500-10,000,000 g/mol. These columns are packed with a

stationary phase consisting of ~10 μm gel particles which are composed of a highly

crosslinked polystyrene/divinylbenzene matrix. These columns are organic GPC

columns, compatible with most organic mobile phase solvents.

Data collected by refractive index (RI) detection was used for characterization of the

molecular weight distribution, molecular weight moments, and polydispersity of the

samples. The data were analyzed using the Agilent GPC/SEC software v A.02.01. A

calibration curve was prepared using polystyrene standards with molecular weights

between approximately 500 and 10,000,000 g/mol. A measured amount of the material

was transferred to a glass vial with a PTFE lined screw cap. An amount of toluene

sufficient to produce a sample concentration of 5 mg/ml was added to each sample,

which were then mixed using gentle agitation at a temperature of 30 °C overnight. All

samples were clear and colorless. The samples were filtered through 0.45 µm PTFE

syringe filters into autosampler vials, filled to the shoulder. Three autosampler vials

were prepared of the samples for triplicate injection purposes. Molecular weight

moments and polydispersity index (PDI) were calculated by Agilent GPC/SEC Software

(v A.02.01) as:

$Mn = \Sigma M_i N_i / \Sigma N_i$

Where Mn is the number molecular weight; M_i is the molecular weight of a chain and N_i

is the number of chains of that molecular weight.

$Mw = \Sigma M_i^2 N_i / \Sigma M_i N_i$

Mw is the weight average molecular weight. In this molecular weight value the more

massive chains contribute more to the molecular weight average.

$PDI = Mw/Mn$

PDI is the polydispersity index.

Origami DNA

The origami folding mixture comprised 208 staples, each 200 nM (Table in S1 Table)

and a scaffold (20 nM), which was a single-stranded DNA p7249 isolated from

M13mp18 (7,249 nucleotides) in Tris buffer (5 mM, pH ~ 8.2, with 1 mM EDTA, 20 mM

$MgCl_2$, and 5 mM NaCl.

Droplet formation was done using PDMS radial chips that empty droplets of aqueous

phase from 20 μm channels into an annular oil flow channel of 50 μm, as previously

described by Paegel and Joyce [10]. The continuous phase was a 2% (v/v) of a

fluorinated surfactant (a-R_2) in Fluid B. The continuous phase was pumped at a rate of 5

μL/min while the aqueous phase was pumped at a rate of 7 μL/min.

The origami mixture, both bulk (as a positive control) and emulsified, were placed in a

thermal cycler at 65 °C for 10 minutes and then cooled to 60 °C at 0.1° C/s. After this

hold, the temperature was lowered by 0.5 °C steps (0.1 °C/s rate) and held at the new

temperature for 30 minutes until 40 °C was reached. At the end of the cooling steps the

emulsion was centrifugated for 5 minutes at 5,000 xg. Then, 25 μL of the origami

reaction were mixed with the provided 6X loading buffer provided with the kit and loaded

in an agarose gel 0.5 X Tris-borate EDTA buffer with ethidium bromide and 6 mM

$MgCl_2$.

Six-nucleotide PCR with Artificially Expanded Genetic Information

Systems (AEGIS)

An aqueous solution holding all components required for a PCR was prepared,

consisting of: (a) primers (20 nM each) 5'- GACGGACTGCCTATGAG-3 and 5'-

GAGGCGATCGCAGTATC-3'; (b) double stranded template (2 x 10^{-7} μM):

5'- GACGGACTGCCTATGAGCAGTT**Z**AAAAG**Z**TATGATACTGCGATCGC CTC-3' and

5'- GAGGCGATCGCAGTATCATA**P**CTTTT**P**AACTGCTCATAGGCAGTCCGTC-3'; (c)

substrates, dNTPs, dZTP, and dPTP (0.2 mM each), (d) Evagreen 2X; (e) a variant of

Taq DNA polymerase fused to the DNA binding protein of *Sulfolobus solfactaricus*

Sso7d-*Taq*(Δ1-280) [R587Q E626K I707L E708K A743H E832G]) at 7.1 x 10^{-2} µM; and

(f) buffer, with 20 mM Tris-HCl, pH 8.4; 10 mM $(NH_4)_2SO_4$; 10 mM KCl; 2 mM $MgSO_4$;

0.1% Triton® X-100.

The PCR mixture (100 µL) was emulsified along with 300 µL of a fluorinated fluid with

density 1.009 g/mL that contained 2% (v/v) surfactant (a-R_2). The fluid was prepared by

mixing 1 mL of fluid B with 4 mL of the HMW fluid (protocol 1). The mixture of two

phases was placed in a Safe-Lock Tube with and a 6 mm stainless steel bead. The tube

was then fitted in a 96-well storage plate and secured between the top and bottom

plates of TissueLyser II (QIAGEN). The components were then mixed for 10 seconds at

15 Hz followed by 7 seconds at 17 Hz. Then, 50 µL of emulsion were transferred to

PCR tubes with an optical lid by triplicate. The PCR used the following cycle: 92 °C for

30 seconds 40 cycles: [92 °C for 10 seconds; 48 °C for 15 seconds; 72 °C for 20

seconds] and acquired fluorescence after each cycle using a Lightcycler® 96 (Roche

Life Science).

291 **Taqman® assay in droplets**

An aqueous solution containing the components of a Taqman® assay reaction was

prepared to contain:

• Template: 5'-CAGCAGTGCCAGCAGAACAAAGGTATTCATCTTAGTGA**P**GTGCGC

AGTCAGCTCACTACT-3', at 0.4 µM concentration.

• Primer: 5'-AGTAGTG AGCTGACTGCGC-3', at 0.2 µM concentration; and

• Probe: 5'- FAM-ATGAATACC-ZEN-TTTGTTCTCTGCTGG CAACTGCTG-3'

The other components of the reaction mixture were: (a) substrate dNTPs and dZTP,

each at 0.2 mM; (b) buffer at 10 mM Tris pH 8.3, 1.5 mM $MgCl_2$, 50 mM KCl; and (c)

enzyme, a variant of *Taq* DNA polymerase [R587Q, E832C], 6 pmol/50 µL reaction.

The aqueous mixture (100 µL) was emulsified along with 300 µL of a fluorinated fluid

with density 1.009 g/mL that contained 2%(v/v) surfactant (a-R_2). The fluid was

prepared by mixing 1 mL of fluid B with 4 mL of the HMW fluid (protocol 1). The tube

containing the two phases was then fitted in a 96-well storage plate and secured

between the top and bottom plates of TissueLyser II (QIAGEN). The components were

then mixed for 10 seconds at 15 Hz followed by 7 seconds at 17 Hz. Then, 50 µL of

emulsion were transferred to PCR tubes with an optically clear lid and placed in the

following cycle: 40 cycles of: [95 °C for 8 seconds; 62 °C for 24 seconds] and acquired

fluorescence after each cycle using a Lightcycler[®] 96 (Roche Life Science).

Rolling circle amplification (RCA) in droplets

An aqueous mixture comprising all of the components for a RCA reaction was

prepared to include: 1X Phi29 buffer (New England Biolabs), which has 50 mM Tris-HCl

at pH 7.5, 10 mM $MgCl_2$, 10 mM $(NH_4)_2SO_4$, and 4 mM DTT (@ 25 °C); (b)

triphosphates, dATP, dCTP, dTTP, dGTP, 0.2 mM each; primer at 0.8 µM, having the

sequence 5'-CAGGGCTGGGCATAGAAGTCAGGGCAGA-3'; polymerase, Phi29 0.1

U/µL, with BSA 0.2 µg/µL; circular ssDNA template molecule at 2.5 µg/µL. The circular

ssDNA template was prepared by circularizing: P-5'TATGCCCAGCCCTGTA

AGATGAAGATAGCGCACAATGGTCGGATTCTCAACTCGTATTCTCAACTCGTAT

TCTCAACTCGTCTCTGCCCTGACTTC-3' with CircLigase™ (Lucigen) according to the

manufacturer protocol. Non-circularized material was degraded with Exonuclease I (*E.*

coli) according to the manufacturer protocol as well.

The aqueous mixture holding all the components necessary for RCA was emulsified

by placing aqueous mixture (100 µL) along with 300 µL of a fluorinated fluid with density

1.009 g/mL that contained 2%(v/v) surfactant (a-R_2). The fluid was prepared by mixing 1

mL of fluid B with 4 mL of the HMW fluid (protocol 1). The tube containing the two

phases was then fitted in a 96-well storage plate and secured between the top and

bottom plates of TissueLyser II (QIAGEN). The components were then mixed for 10

seconds at 15 Hz followed by 7 seconds at 17 Hz. Then, 50 µL of emulsion were

transferred by triplicate to PCR tubes with an optically clear lid. Fluorescence was

acquired after each minute using a Lightcycler[®] 96 (Roche Life Science).

Expression and purification of the DNA polymerase variants

A plasmid (pJExpress414, DNA 2.0) containing the gene encoding the *Taq* DNA

polymerase variant of interest was expressed in *E. coli* C43(DE3) (37 ºC, overnight

growth, IPTG 0.5 mM) in LB media (50 mL). The next morning, cells were pelleted (~

0.75 g) in a refrigerated centrifuge for 10 minutes at 5,000 x g and stored at -20º C. The

pellet was resuspended in 2.5 mL of Tris 50 mM; glucose 50 mM; EDTA 1 mM; pH 8.0

and heat-shocked at 75 ºC for 10 minutes, then mixed with 3.75 mL of BugBuster®

master mix (Novagen) for 20 minutes at room temperature. The lysate was pelleted in

1.5 mL tubes, at 21,000 xg for 5 minutes and the supernatant was mixed with NiNTA

resin (1.5 mL of resuspended resin washed and resuspended in 4 mL of Lysis buffer:

Tris HCl, 20 mM pH 8.0; NaCl 500 mM, imidazole 10 mM). The lysate and the resin

were then incubated and gently spun at 4 ºC for 1 h.

The lysate was then loaded on a column and washed with: (a) 2 mL wash: Tris, 20

mM; NaCl, 1 M; followed by (b) 1 mL wash: Tris, 20 mM; NaCl, 150 mM; followed by (c)

2 mL wash: Tris, 20 mM; NaCl, 500 mM; imidazole, 20 mM; and (d) eluted with elution

buffer: 1 mL Tris HCl, 10 mM, pH 8.0, NaCl 250 mM, imidazole 500 mM. Buffer was

exchanged by ultracentrifugation (AMICON, 15 mL, 50,000 MW cutoff) to final storage

buffer, which was 10 mM Tris pH 8.0; 100 mM KCl; 0.5 mM DTT; 0.1 mM EDTA; 0.5%

Tween 20; 0.5 % Igepal; glycerol 50%. Protein concentration was measured using

Pierce™ BCA Protein Assay Kit, following the manufacturer recommendations.

Results

Fluorine has an atomic mass of 19, meaning fluorinated molecules are intrinsically

denser than water. However, this greater atomic mass can be partly offset by the larger

mean volumes of CF_2 (38 Å^3) and CF_3 (92 Å^3) groups relative to CH_2 (27 Å^3) and CH_3

(54 Å^3) [31], both less dense than water. Therefore, we reasoned that fluorous oils

having a density of water might be obtained by balancing their fluorinated components

with alkane components. This balancing must also consider the density of silicon (Si =

28 g/mole) since cyclotrisiloxanes are part of the polymerization mixture.

With these considerations, we explored methods to prepare low-density fluorous oils

by reacting siloxanes having both alkane and trifluoromethylalkane side chains,

specifically 1,3,5-trimethyl 1,3,5-tris(3,3,3-trifluoropropyl)-cyclotrisiloxane and

hexamethylcyclotrisiloxane (Fig 2). It was taken into consideration that the growth of

the polymeric chain must be limited since high molecular weight molecules will increase

the viscosity of the fluid. For this purpose the chain termination component

(hexamethyldisiloxane) plays an essential role.

Ring-opening polymerization

Acid-catalyzed ring-opening polymerization following protocol 1, produced

polysiloxanes with bimodal molecular weight distribution (Fig 4). Protocol 2 produced

two fluids with different densities which spontaneously separated. Interestingly, each of

these fluids exhibits a bimodal molecular weight distribution as well (Fig 5). Following

protocol 1, fluid A was separated by distillation using a Kugelrohr apparatus. Obtaining

15 mL of the lower molecular weight fraction (150 ºC, 23 mm Hg) with a density of

1.0565 g/mL. The remaining fluid (~ 53 mL) consists of a high molecular weight fraction

with density 1.031 g/mL; this remained undistilled up to 200 ºC at 23 mm Hg). Table 1

lists molecular weight values for different fractions.

Figure 4. Molecular weight distribution of polysiloxanes produced via protocol 1.

Ring-opening polymerization following "protocol 1" produced polysilioxanes with bimodal

distribution. These two peaks can be separated by distillation under reduced pressure

with a high molecular weight peak (Mp ~ 9,400 g/mol) and a low molecular weight peak

(Mp ~ 300 g/mol). The low molecular weight fraction contains a higher concentration of

fluorinated monomers estimated by ^{1}H-NMR and is capable of dissolving the fluorinated

surfactants. Peak 1 corresponds to the higher molecular weight peak (rightmost) and

peak 2 corresponds to the lower molecular weight peak (leftmost). S4 Fig. shows an

overlay of two gel permeation chromatography runs of the two distinctive fractions

separated by distillation.

Figure 5. Molecular weight distribution of polysiloxanes produced via protocol 2.

Ring-opening polymerization following "protocol 2" produced two liquid polysiloxanes

that spontaneously separate in two phases with different densities and are referred as

fluid C (red) and fluid D (blue). Each fluid exhibits bimodal molecular weight distribution.

Table 1. Summary of molecular weight moments and polydispersity.

sample	Mp [g/mol]	Mn [g/mol]	Mw [g/mol]	PDI
Fluid A	9,404 ± 57.7	1748 ± 31.2	10,126 ± 83.5	5.793 ± 0.058
Fluid A peak 1	10,321 ± 34.6	3,206 ± 486	11,478 ± 74.0	3.637 ± 0.561
Fluid A peak 2	321 ± 2.08	230 ± 2.65	305 ± 2.00	1.326 ± 0.008
Fluid C	6,412 ± 64	2,064 ± 11	6,266 ± 116	3.04 ± 0.06
Fluid C peak 1	6,412 ± 64	4,549 ± 34	7,529 ± 144	1.66 ± 0.019
Fluid C peak 2	626 ± 6	597 ± 3	637 ± 3	1.07 ± 0.008
Fluid D	645 ± 4	1,722 ± 12	6,543 ± 119	3.80 ± 0.07
Fluid D peak 1	7,178 ± 47	4,892 ± 23	8,522 ± 70	1.74 ± 0.009
Fluid D peak 2	645 ± 4	611 ± 4	661 ± 4	1.08 ± 0.003

Reported molecular weight moments and polydispersity from the overall chromatogram,

as average +/- one standard deviation. Molecular weights are reported in polystyrene

equivalents. Fluid A peak 1 is referred as high molecular weight fraction (HMW) and

Fluid A peak 2 referred as low molecular weight fraction (LMW). $Mn = \Sigma M_i N_i / \Sigma N_i$, where

Mn is the number molecular weight; M_i is the molecular weight of a chain and N_i is the

number of chains of that molecular weight. $Mw = \Sigma M_i^2 N_i / \Sigma M_i N_i$, where Mw is the weight

average molecular weight. In this molecular weight value the more massive chains

contribute more to the molecular weight average. PDI is the polydispersity index. PDI =

Mw/Mn.

Figure 6. [1]NMR analysis of fluorosilicone polysiloxanes. Overlay of the ^{1}HNMR of

the low molecular weight (blue) and the high molecular weight (red) fraction samples

indicating the assigned peaks.

^{1}HNMR analysis

Resonances with chemical shifts between 0.0 and 0.3 ppm were assigned to Si-CH$_3$

(labeled "a" in Fig 6). These signals arise from both fluorinated and non-fluorinated

monomers. Resonances with chemical shifts between 0.7 and 0.9 ppm were assigned

to the methylene groups attached to Si (α-CH$_2$-, labeled "b" in Fig 6). Resonances with

chemical shifts between 1.9 and 2.2 ppm were assigned to the methylene beta to the Si

(β-CH$_2$-, labeled "'c" in Fig 6) for the fluorinated monomers that contained -CH$_2^{\alpha}$-CH$_2^{\beta}$-

CF$_3$.

The ratios of non-fluorinated monomer to fluorinated monomer were calculated using

the integrals from the β protons (denoted by "c") and the Si-CH$_3$ protons (denoted by

"a"). The following equation was used to determine the monomer ratio:

$$\frac{\text{Non} - \text{fluorinated monomer}}{\text{Fluorinated monomer}} = \frac{(Aa - 3)/6}{Ac/2}$$

422 Here, A$_c$ is the integration area of the peak for the β-CH$_2$- protons and A$_a$ is the

423 integration area of the peak for the Si-CH$_3$ protons. The integration values and

424 monomer ratios are summarized in Table 2.

426 **Table 2. Integration of peaks used for determination of the ratio of non-fluorinated monomer:**

427 **fluorinated monomer.**

sample	β-CH$_2$	Si-CH$_3$	non-fluorinated monomer: fluorinated monomer
Fluid A peak 2 (LMW)	2	18.3	2.6 : 1
Fluid A peak 1 (HMW)	2	96.3	15.6 : 1

Values for samples HMW: high molecular weight and LMW: low molecular weight. ^{1}HNMR β-CH$_2$

integral was set to the value 2. ^{1}HNMR data is representative of several trials.

The integral of the resonances assigned to the Si-CH$_3$ units (0.0 to 0.3 ppm) is

inversely proportional to the fraction of fluorinated monomers present in the fluid. It was

observed that fractions with higher fluorinated monomers exhibited lower viscosity. As

expected, the fractions with a higher degree of fluorination were capable of solubilizing

the nonionic fluorinated surfactants. Figs 7 and 8 show ^{19}FNMR and ^{1}HNMR of

homogeneous solutions of the surfactants in the low molecular weight fraction (Fluid B,

protocol 1). These solutions remained homogeneous for at least 10 days. The NMR

spectra show the distinctive signals that arise from the surfactants solubilized to 4%

(v/v). Table 3 shows different values of density, viscosity and proportion of non-

fluorinated to fluorinated monomer compositions in the fluorinated polysiloxanes.

447 **Table 3. Viscosity, density and other properties measured on fluorinated polysiloxanes.**

sample	density (g/mL)	Viscosity (cSt)	^{1}HNMR β-CH2 integral	^{1}HNMR Si-CH3 integral	MW (g/mol)	PDI	non-fluorinate fluorinated monomer
Fluid A peak 2	1.031	n/d	2	18.3	305	1.3	2.55 : 1
Fluid A peak 1	1.0565	n/d	2	96.3	11,478	3.6	15.55 : 1
HMW fluid	0.986	67	2	58.0	10,126	5.8	9.17 : 1
Fluid C	1.0457	6.06	2	33.98	6,266	3.04	5.16 : 1
Fluid D	1.1347	10.8	2	12.24	6,543	3.8	1.54 : 1
Fluid B *	1.1397	4.5	2	11.48	n/d	n/d	1.41 : 1

Summarized viscosity and molecular weight analysis for fluorinated polysiloxane samples. Reported

viscosity as fitted using a Newtonian model. Determined by Cambridge Polymer Group using a TA

Instruments DHR-2 rheometer. Reported molecular weight moments and polydispersity from the

overall chromatogram, as average +/- one standard deviation. Molecular weights are reported in

polystyrene equivalents. Fluid B* was prepared following protocol 1 but with a shorter time of

reaction obtaining a fluid with lower viscosity but with higher density and higher proportion of

fluorinated monomers. ^{1}HNMR **β-CH$_2$** integral was set to the value 2. Some tests not performed are

indicated as "not determined" n/d.

Figure 7. ^{19}FNMR overlays showing the presence of the surfactant with the Hx$_f$

hydrophobe CF$_3$CF$_2$CF$_2$CF$_2$CH$_2$CH$_2$- dissolved in the low molecular weight fluid

(fluid B). (A) A single peak that comes from the C**F$_3$**CH$_2$CH$_2$- from the fluorinated fluid.

(B) Four peaks that correspond to the fluorine of the Hx$_f$ hydrophobe

C**F$_3$CF$_2$CF$_2$CF$_2$**CH$_2$CH$_2$-. (C) ^{19}FNMR of a homogeneous 4% solution (v/v) of the

surfactant in the fluorinated fluid exhibiting the signals from both components.

Figure 8. ^{1}HNMR overlays showing the presence of the surfactant with the Pr$_f$

hydrophobe CF$_3$CH$_2$CH$_2$- dissolved in the low molecular weight fluid (fluid B). (A)

^{1}HNMR of the fluid without surfactant. (B) ^{1}HNMR of a 4% (v/v the fluid with surfactant.A

single peak that comes from the CF$_3$CH$_2$CH$_2$- from the fluorinated fluid. The

characteristic signals of the -(CH$_2$CH$_2$-O)- can be observed at 3.4-3.8 ppm.

Droplet formation

Droplets shown in this work were made using two methods: using microfluidic devices

or by shaking using a QIAGEN TissueLyser II. Fig 9 shows droplets produced with a

radial microfluidics chip. Fig 10 shows droplets formed by shaking 300 µL of the

fluid/surfactant with 100 µL of the aqueous phase in a Safe Lock tube with a 6 mm

stainless steel bead.

Figure 9. Transmission microscope images of droplets containing oligos with a

FAM fluorescent molecule or a Black hole quencher (BHQ). The fluorinated fluid

(fluid B) with 1% of surfactant (b-R$_1$) was pumped at 10 µL/min. Aqueous phase

contained 5 µM of 5'-CTGCTCATAGG CAGTCCGTCA-BHQ-3' or

5'-FAM-TGACGGACTGCCTATGAGCAG-3' in 20 mM Tris-HCl, pH 8.4; 10 mM

(NH$_4$)$_2$SO$_4$; 10 mM KCl; 2 mM MgSO$_4$; 0.1% Triton® X-100. Aqueous phase was

pumped at 2 µL/min. (A) Droplets carrying oligo with Black Hole Quencher (BHQ). (B)

Droplets carrying oligo with FAM. (C). Droplets carrying BHQ placed on the left side of the

glass slide and droplets carrying FAM placed on the right hand side of the slide. (D)

After being in contact for 10 minutes no fusion is observed. Scale bar is 400 μm.

Pictures are representative of several trials.

Figure 10. Emulsion made with fluid C (protocol 2). Left: transmission microscope

image of droplets. Scale bar is 200 μm. Right: picture of the emulsion formed by

shaking 100 μL of buffer and 300 μL of fluid C with 2% of the surfactant a-R$_2$ containing

the Hx$_f$ hydrophobe. The emulsion is formed by shaking the contents in a Snap-Cap

Microcentrifuge Biopur™ Safe-Lock™ Tube containing a 6 mm stainless steel bead.

The tube was fitted in a TissueLyser II and shaken for 10 seconds at 15 Hz followed by

7 seconds at 17 Hz. Scale bar is 400 μm. Pictures are representative of several trials.

Next, we challenged the emulsions prepared with these fluid/surfactant mixtures to

host processes that involve both DNA and enzymes, all useful in biomolecular sciences,

nanotechnology: (a) Assembly of origami DNA nanostructures inside droplets

suspended in the fluorinated oil. (b) PCR amplification of 6-letter DNA templates inside

droplets suspended in the fluorinated oil, including those built from an AEGIS DNA

alphabet. (c) Generation of fluorescent signals inside droplets suspended in the

fluorinated oil using a Taqman® assay, also with six-letter DNA real-time PCR.

(d) Generation of fluorescent signals inside droplets suspended in the fluorinated oil

from the formation of RCA products.

Origami DNA

An origami kit obtained from Tilibit Nanosystems that assembles to form a cuboid of dimensions 61 nm x 8 nm x 52 nm with an aperture of 9 nm x 15 nm was set up as suggested by the manufacturer. The formation of the nanostructure was verified by its distinctive shift in migration compared with the scaffold when electrophoresed in a 2% agarose gel in 0.5 X TBE with ethidium bromide and 6 mM $MgCl_2$. The migration pattern of the scaffold DNA and a correctly assembled nanostructure is shown in S8 Fig. The purified nanostructure has been characterized by Transmission Electron Microscopy (S9 Fig.). Our results showed that both the emulsified and non-emulsified origami reaction produced a nanostructure with the expected migration pattern (Fig 11). The result shown in Fig 11 comes from droplets prepared using microfluidics as described in the experimental section. This experiment was repeated preparing the emulsions using a TissueLyser II (QIAGEN) without noticeable difference between the methods of emulsification (S5 Fig.).

Figure 11. DNA electrophoresis in agarose (2%) showing the formation of origami structures in droplets. The origami products were run in 0.5 X Tris-borate EDTA buffer with ethidium bromide and 6 mM $MgCl_2$. The origami structure folded is called "nanostructure PF-2, cuboid with large aperture" from Tilibit Nanosystems. The scaffold, a single-stranded DNA type p7249 isolated from M13mp18 of length 7,249 bases. The staples are a mixture of 208 oligos (S1 Table 1). A sample of the mixture of scaffold and staples not annealed is run for comparison. The origami folded properly shows a distinctive migration on the gel (see Figs S8 and S9 for reference). Annealing

was done by incubating at 65 °C for 10 minutes then cooled down from 60 °C to 40 °C

at a rate of 1 °C per hour.

AEGIS PCR with 6-Letters

To demonstrate that droplets suspended in the iso-dense fluorinated oil had thermal

stability adequate to support PCR and, in particular, PCR containing AEGIS bases, a

double stranded DNA molecule with 49 bp containing the AEGIS pair Z:P (Fig 1) was

used as template. The enzyme used to amplify this was a derivative of the *Taq* DNA

polymerase where the amino acids 1-280 were deleted (removing the exonuclease

domain), with the N-terminus of the catalytic domain fused to a processivity enhancing

domain from *Sulfolobus solfataricus*. The *Taq* variant has 6 mutations, two specific for

enhancing the incorporation of the pair **Z:P** (R587Q and E832G). The enzyme is

described as: Sso7d-*Taq* (Δ 1-280) R587Q E626K I707L E708K A743H E832G.

Progress of the PCR was monitored by observing the fluorescence of Evagreen®,

which intercalates into double-stranded PCR amplicons. Fig 12 shows real time PCR

fluorescence signals arising from the PCR reaction. As a control a PCR done in bulk

aqueous solution shows comparable fluorescence signals to the ones that come from

water droplets emulsified in iso-dense fluorinated oil. These results showed that neither

the surfactant nor the fluorinated oil had any measurable impact on the progress of the

PCR. This is consistent with the orthogonality of the fluorinated oil and the surfactant

with respect all biological molecules involved in the PCR.

Figure 12. Real time PCR showing emergence of fluorescence from intercalated

Evagreen® without emulsification (blue lines) and in the emulsified PCR (red

lines). The aqueous phase was emulsified by mixing 100 µL of aqueous phase mixed

with 300 µL of fluorinated oil (1 volume of LMW fraction and 4 volumes of the HMW

fraction, see protocol 1) with 2% of surfactant (a-R_2). Assays done by triplicate.

Taqman® assay

One standard way to detect DNA is a Taqman® assay. Here, DNA polymerase from

Thermus aquaticus degrades the downstream strand using its 5'-3' exonuclease activity

displacing a probe from the template, cleaving the probe in the process. This cleavage

separates a fluorescent reporter (here, fluorescein, FAM) from one end of the probe

from a fluorescence quencher at the other end of the probe, to give a fluorescent signal.

Here, we adapted the Taqman® assay to detect a target analyte that contained AEGIS

dZ and dP (Fig 1). As before, the aqueous phase was emulsified by mixing 100 µL of

aqueous phase mixed with 300 µL of fluorinated oil (1 volume of LMW fraction and 4

volumes of the HMW fraction, see protocol 1) with 2% of surfactant (a-R_2). Emulsions

were made by shaking using a QIAGEN TissueLyser II (15 Hz for 10 seconds followed

by 17 Hz for 7 seconds) in a Snap-Cap Microcentrifuge Biopur™ Safe-Lock™ tube

containing a 6 mm stainless steel bead. Again, output was essentially the same as

observed in bulk Taqman® assays (Fig 13). The *Taq* DNA polymerase variant used

contains two mutations (R587Q, E832C) that favor the incorporation of the Z:P pair

Figure 13. Taqman® assay in droplets. Top: Scheme of the Taqman® assay

containing AEGIS (dZ:dP pair hydrogen bonding shown). Bottom: Real-time

fluorescence detected from a probe. The probe contains a 5′ fluorophore: 6-

carboxyfluorescein (6FAM) and is double-quenched with: 3′ Iowa Black™ (IABk) and a

proprietary internal ZEN quencher (IDT). When *Taq* [R587Q E832C] polymerase places

a dZ opposite dP and the 5'-3' exonuclease of *Taq* polymerase cleaves the probe

eventually releasing a fluorescent molecule. The blue line is the fluorescence from a

non-emulsified reaction. The red line corresponds to the signal from the emulsified

reaction. The emulsion was made by mixing 100 µL of aqueous phase with 300 µL of a

fluorinated oil with 2% (v/v) fluorinated surfactant as shown on Fig 2. Mixed in QIAGEN

TissueLyser II in the presence of a 6 mm stainless steel bead at 15 Hz for 10 seconds

followed by 17 Hz for 7 seconds using an Eppendorf Safe-Lock Tube (2 mL) containing

a stainless steel ball. Assays were done by triplicate.

592   RCA in droplets

RCA works by having a circular template, a primer that binds to that circular template,

and a strand displacing polymerase that extends that primer, displacing already

synthesized DNA as it proceeds around the circle. Here, the aqueous phase used to

prepare the droplets contains a circularized template 96 nucleotides around, a primer

complementary to the circular template, and dNTPs. The polymerase was Phi29 DNA

polymerase. The progress of the RCA was followed by measuring fluorescence emitted

by an intercalating fluorescent dye (EvaGreen®) in a Light Cycler over a period of 1

hour (Fig 14).

Figure 14. Amplification curves obtained using the LightCycler96 for RCA amplification in droplets. Fluorescence detection (EvaGreen®) is acquired after each two step cycle [37 °C for 30 seconds - 37 °C for 30 seconds followed by aquisition] x 60 cycles. Blue lines correspond to the reaction that was not emulsified. Red lines correspond to the emulsified reaction. Assays done by triplicate.

Discussion

The growing interest in synthetic cells [51] matches a growing interest in engineering enzymes for synthetic biology using directed evolution [52, 53] [54]. For example, Tawfik and Griffiths [26] developed a method to link genotype and phenotype in droplets of water emulsified in oil called "Compartmentalized Self-Replication" (CSR). This strategy was adapted in the Holliger laboratory for the directed evolution of DNA polymerases [10].

However, various laboratories have reported difficulties in reproducing CSR procedures. One of the first problems identified was associated to the surfactant Span 80® [55]. It is very likely that Span 80®, which is derived from animal fat, carries in uncontrolled amounts a problematic contaminant. Indeed, the Holliger group reports the need for an antioxidant to avoid oxidation due to peroxide contaminants in Span 80® [35]. Thus, while results are possible with surfactant mixtures containing Span 80®, these are hit-or-miss, and has become known in the community as problematically irreproducible.

For this reason, many have turned to synthetic materials and a third liquid phase, the

"fluorous phase". Kobayashi and Owen reported some time ago the synthesis of non-

ionic fluorosilicone surfactants with 3,3,3-trifluoropropyl and 3,3,4,4,5,5,6,6,6-

nonafluorohexyl side chains with poly(oxyethylene) hydrophiles [50].

Here, balancing the mixture of hydrocarbon-carrying silanes, intrinsically less dense

than water, with fluorohydrocarbon-carrying silanes, intrinsically more dense than water,

yielded mixtures that had densities essentially identical to the density of water. As the

density of water can change with different amounts of solutes, the density of the

fluorinated oils described here can be changed by mixing the fractions, separated by

distillation, in different ratios to match the desired density.

The fluorinated oils described here have been used to encapsulate different

biochemical reactions such as DNA origami folding, PCR, Taqman[®] assay and RCA.

We found no negative impact of the encapsulation. All of these biochemical reactions

worked as well in these iso-dense fluorinated oil-surfactant systems as their non-

emulsified analogs. Thus, they add a significant and important new resource for

nanotechnology, directed evolution and synthetic biology.

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Supporting information

S1 Table 1. Sequences of oligos used as staples for origami structure PF-2 cuboid with large aperture.

List of oligos used as staples in Origami DNA folding experiment.

S1 Figure. PCR in emulsion using different batches of Span$^{®}$ 80.

S2 Figure. Dark precipitates observed in Span$^{®}$ 80.

S3 Figure. Example of synthesis of fluorinated nonionic surfactant a-R$_2$.

S4 Figure. Overlay of molecular weight distribution of the two fractions separated by distillation after ring-opening polymerization following protocol 1.

S5 Figure. Origami fold in droplets using a QIAGEN TissueLyser II.

S6 Figure. Raw image of S5 Figure.

S7 Figure. Raw image of Fig 11.

S8 Figure. DNA electrophoresis of cuboid with large aperture from Tilibit Nanosystems.

S9 Figure. Transmission Electron Microscopy (TEM) of a correctly assembled DNA origami cuboid with large aperture from Tilibit Nanosystems.

S10 Figure. Droplets made using a microfluidic device (T-junction).

S1 File. MW distribution. Molecular weight distribution data for Fig 4 and S4 Fig.

S2 File. MW distribution. Molecular weight distribution data for Fig 5.

pyDDA   **puAAD**

unshared pair of electrons

Z:P

pyDAA   **puADD**

unshared pair of electrons

C:G

Hexamethylcyclotrisiloxane

1,3,5-trimethyl 1,3,5-tris (3,3,3-trifluoropropyl)cyclotrisiloxane

Hexamethyldisiloxane

Amberlyst® 15

6-FAM   IABk

5' ──────────────────────   5'─────────────────3'
3' ────────────────── AEGIS ──────────────────────────

6FAM   ZEN   IABk
5'-AGTAGTGAGCTGACTGCGC   ATGAATACCTTTGTTCTGCTGGCACTGCTG-3'
3'-TCATCACTCGACTGACGCGTG**Z**AGTGATTCTACTTATGGAAACAAGACGACCGTGACGAC-5'