Chronic PPARγ Stimulation Shifts Amyloidosis to Higher Fibrillarity but Improves Cognition

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Abstract

Background: We undertook longitudinal β-amyloid positron emission tomography (Aβ-PET) imaging as a translational tool for monitoring of chronic treatment with the peroxisome proliferator-activated receptor gamma (PPARγ) agonist pioglitazone in Aβ model mice. We thus tested the hypothesis this treatment would rescue from increases of the Aβ-PET signal while promoting spatial learning and preservation of synaptic density.

Methods: PS2APP mice (N=23; baseline age: 8 months) and App^{NL-G-F} mice (N=37; baseline age: 5 months) were investigated longitudinally for five months using Aβ-PET. Groups of mice were treated with pioglitazone or vehicle during the follow-up interval. We tested spatial memory performance and confirmed terminal PET findings by immunohistochemical and biochemistry analyses.

Results: Surprisingly, Aβ-PET and immunohistochemistry revealed a shift towards higher fibrillary composition of Aβ-plaques during upon chronic pioglitazone treatment. Nonetheless, synaptic density and spatial learning were improved in transgenic mice with pioglitazone treatment, in association with the increased plaque fibrillarity.

Conclusion: These translational data suggest that a shift towards higher plaque fibrillarity protects cognitive function and brain integrity. Increases in the Aβ-PET signal upon immunomodulatory treatments targeting Aβ aggregation can thus be protective.

1. Introduction

With its exponentially increasing incidence as a function of age, Alzheimer's disease (AD) has become the most common cause of dementia, and is imposing a significant burden on health care systems of societies with aging populations (1). During the past few decades, research on AD pathogenesis led to the formulation of a model that accumulation of amyloid beta (Aβ)-plaques and neurofibrillary tangles, the histologically characterizing hallmarks of AD (2), triggers a cascade of neurodegenerative events, leading to disease progression (3). Additionally, novel emerging evidence indicates that neuroinflammation plays an important role in pathogenesis and progression of AD and many other neurodegenerative diseases (4; 5). Microglia, the resident macrophages of the central nervous system (CNS), innate immune system, continuously survey the brain parenchyma for pathogens or cellular debris, provide factors for tissue repair, and contribute to plasticity of neuronal circuits by protecting and remodeling of synapses. In AD, microglial cells are activated by Aβ-deposition and migrate towards the Aβ-plaques (6). The activated microglial cells are then able to bind and phagocytize soluble Aβ, and to some degree also the fibrillary Aβ aggregates, as part of the increased inflammatory response (4). However, others report that Aβ-recognition receptors on microglia downregulate during the progression of AD, such that microglial cells eventually undergo senescence, characterized by reduced phagocytosis of Aβ-aggregates (7); with time, the decreased microglial activity is permissive to expansion of fibrillar amyloidosis (8; 9). The dystrophic phenotype of previously activated microglial cells also manifests in morphological changes, such as loss of ramification, decreased fiber mobility, swelling or fragmentation of the cytoplasm; moreover, senescent microglia show a threefold higher mortality rate compared to non-plaque associated microglial cells (9–11; 6). A high proportion of dystrophic microglia were observed in human AD brain *post mortem* (11). These observations have led some to speculate that the microglial response is overwhelmed by the massive Aβ-deposition occurring in advanced AD, such that their chronic activation has a detrimental impact on disease progression (12; 7).

It might follow that treatment with anti-inflammatory drugs should alleviate AD progression. However, clinical trials using non-steroid anti-inflammatory drugs (NSAID) to suppress chronic inflammation have delivered inconclusive results (4). Most of such trials failed to show any improvement in cognitive performance in subjects with mild cognitive impairment of AD dementia (13). Pioglitazone is an anti-inflammatory insulin sensitizer widely used to treat hyperglycemia in type 2 diabetes via activation of peroxisome proliferator-activated receptor gamma (PPAR-γ). As an alternative to NSAIDs, treatment with pioglitazone enables microglial cells to undergo a phenotypic conversion from a pro-inflammatory towards an anti-inflammatory, neuroprotective phenotype (14; 15). Furthermore, activation of PPAR-γ in the brains of AD mice initiate a coupled metabolic cycle with the Liver X Receptor to increase

brain apolipoprotein E levels, which promotes the ability of microglial cells to phagocyte and degrade both soluble and fibrillary Aβ (14; 15). However, another study showed that only low-dose PPAR-γ agonist treatment, but not the conventional doses, promotes an Aβ-clearing effect by increasing (LDL Receptor Related Protein 1 (LRP1) in human brain microvascular endothelial cells (HBMECs) (16). Increasing LRP1 expression in the hippocampus alleviated learning and memory impairments in a mouse model of AD (17). Despite this compelling preclinical evidence, a meta-analysis encompassing nine clinical studies did not compelling support a beneficial effect of PPAR-γ agonist treatment on cognition and memory in in patients with mild-to-moderate AD (18). Furthermore, a phase III trial of pioglitazone in patients with mild AD was discontinued due to lacking efficacy (19). It remains a conundrum why the translation of PPARγ stimulation into human AD failed, which calls for further investigation to uncover the basis of the seemingly false lead. Conceivably, the efficacy of pioglitazone may be confined to a specific stage of AD, or in cases distinguished by a particular biomarker.

Given this background, we hypothesized that the baseline presentation of microglial activation and Aβ-load and composition would determine the individual efficacy of PPARγ stimulation effect in the progression of AD mouse models. Therefore, we test the prediction that the efficacy of pioglitazone in delaying the progression of spatial learning impairments and Aβ-load in AD model mice would be predictable from the individual baseline findings with Aβ-PET. To test this hypothesis, we undertook serial small animal positron emission tomography (μPET) with the Aβ-tracer [^{18}F]florbetaben (20–22) in two AD mouse models with distinct Aβ-plaque composition. The transgenic PS2APP-line develops dense fibrillary Aβ-plaques with late debit whereas the knock-In mouse model App^{NL-G-F} develops more diffuse oligomeric Aβ-plaques with early debut. Both strains of mice were treated with pioglitazone or vehicle for five months during the phase of main Aβ accumulation. We conducted behavioral assessments of spatial learning and confirmed longitudinal PET findings by immunohistochemical analysis and biochemical analysis, thus aiming to test the hypothesis that response to pioglitazone would depend on the type of Aβ-plaques formed in transgenic mice.

2. Methods and Materials

Study design

Groups of PS2APP and App^{NL-G-F} mice were randomized to either treatment (PS2APP-PIO N=13; App^{NL-G-F}-PIO N=14) or vehicle (PS2APP-VEH N=10; App^{NL-G-F}-VEH N=23) groups at the age of 8 (PS2APP) and 5 (App^{NL-G-F}) months. In PS2APP mice, the baseline [^{18}F]florbetaben-PET scan (Aβ-PET) was performed at the age of eight months, followed by initiation of pioglitazone treatment or vehicle for a period of five months and a follow-up Aβ-PET scan at 13 months. In App^{NL-G-F} mice, the baseline Aβ-PET scan was performed at the age of five month, followed by initiation of pioglitazone treatment or vehicle, for a period of five months. Follow-up Aβ-PET scans were acquired at 7.5 months and ten months of age, which was the study termination in App^{NL-G-F} mice. For all mice, behavioral testing after the terminal PET scan was followed by immunohistochemical and biochemical analyses of randomized hemispheres. The TSPO PET arm of the study and detailed analyses of neuroinflammation imaging are reported in a separate manuscript focusing on the predictive value of TSPO-PET for outcome of PPARγ-related immunomodulation (23). The sample size estimation of the in vivo PET study was based on previous experience and calculated by G*power (V3.1.9.2, Kiel, Germany), assuming a type I error α=0.05 and a power of 0.8 for group comparisons, a 10% drop-out rate per time-point (including TSPO-PET), and a treatment effect of 5% change in the PET signal (23). Shared datapoints between the study arms are indicated.

Animals

PS2APP transgenic, App^{NL-G-F} APP knock-in and wild-type C57Bl/6 mice were used in this investigation. All experiments were performed in compliance with the National Guidelines for Animal Protection, Germany, with approval of the local animal care committee of the Government of Oberbayern (Regierung Oberbayern) and overseen by a veterinarian. The experiments complied with the ARRIVE guidelines and were carried out in accordance with the U.K. Animals (Scientific Procedures) Act, 1986 and associated guidelines, EU Directive 2010/63/EU for animal experiments. Animals were housed in a temperature and humidity-controlled environment with a 12-h light–dark cycle, with free access to food (Ssniff) and water.

The transgenic B6.PS2APP (line B6.152H) is homozygous for the human presenilin (PS) 2, N141I mutation and also the human amyloid precursor protein (APP) K670N, M671 L mutation. The APP and PS2 transgenes are driven by mouse Thy-1 and mouse prion promoters, respectively. This line had been created by coinjection of both transgenes into

C57BL/6 zygotes. Homozygous B6.PS2APP (PS2APP) mice show the first appearance of plaques in the cortex and hippocampus at 5–6 months of age (24). The App^{NL-G-F} mouse line carries a mutant APP gene encoding the humanized Aβ-sequence (G601R, F606Y, and R609H) with three pathogenic mutations, namely Swedish (KM595/596NL), Beyreuther/Iberian (I641F), and Arctic (E618G) (25). Homozygous App^{NL-G-F} mice show first appearance of plaques in the cortex and hippocampus at 3-4 months of age (25). Age-matched C57Bl/6 mice served as controls.

Radiochemistry

[^{18}F]florbetaben radiosynthesis was performed as previously described (22). This procedure yielded a radiochemical purity exceeding 98% and a specific activity of 80 ± 20 GBq/µmol at the end of synthesis.

Aβ-PET Acquisition

Mice were anesthetized with isoflurane (1.5%, delivered via a mask at 3.5 L/min in oxygen) and received a bolus injection [^{18}F]florbetaben 12 ± 2 MBq in 150 µL of saline to a tail vein. Following placement in the tomograph (Siemens Inveon DPET), a single frame emission recording for the interval 30-60 min p.i., which was preceded by a 15-min transmission scan obtained using a rotating [^{57}Co] point source.

Reconstruction

The image reconstruction procedure consisted of three-dimensional ordered subset expectation maximization (OSEM) with four iterations and twelve subsets followed by a maximum *a posteriori* (MAP) algorithm with 32 iterations. Scatter and attenuation correction were performed and a decay correction for [^{18}F] was applied. With a zoom factor of 1.0 and a 128 x 128 x 159 matrix, a final voxel dimension of 0.78 x 0.78 x 0.80 mm was obtained.

Small-Animal PET Data Analyses

Volumes of interest (VOIs) were defined on the MRI mouse atlas (26). A forebrain target VOI (15 mm^3) was used for group comparisons and an additional hippocampal target VOI (8 mm³) served for correlation analysis with spatial learning. We calculated [^{18}F]florbetaben standard-uptake-value ratios (SUVRs) using the established white matter (PS2APP; 67 mm^3; pons, midbrain, hindbrain and parts of the subcortical white matter) and periaqueductal grey (App^{NL-G-F}; 20 mm³) reference regions (27–29).

Water Maze

Two different water maze tasks were applied due to changing facilities between the investigations of PS2APP and App^{NL-G-F} cohorts. We used a principal component analysis of the common read outs of each water maze task to generate a robust index for correlation analyses in individual mice (30). The principal component of the water maze test was extracted from three spatial learning read-outs (PS2APP: escape latency, distance, platform choice; App^{NL-G-F}: escape latency, frequency to platform, time spent in platform quadrant). Thus, one quantitative index of water maze performance per mouse was generated for correlation with PET imaging readouts. The experimenter was blind to the phenotype of the animals.

Water Maze in PS2APP mice:

PS2APP and age-matched wild-type mice were subjected to a modified Morris water maze task as described previously (31–34) yielding escape latency, distance to the correct platform and correct choice of the platform as read-outs. Mice had to distinguish between two visible platforms, one of which was weighted such that it would float when the mouse climbed on (correct choice), while the other would sink (wrong choice). The correct platform was always located at the same spot in the maze, while the wrong platform, as well as the site from which the mice were released into the maze, were varied in a pseudorandom fashion. Visual cues on the walls of the laboratory provided orientation. Trials were terminated if the mouse had failed to reach one of the platforms within 30 sec (error of omission). In this case, or in case of a wrong choice, the experimenter placed the mouse on the correct platform for 30 sec. After a three-day handling period, water maze training was performed on five consecutive days, with five trials per day, which were conducted 2-4 minutes apart. Memory performance was assessed by measuring the escape latency at each day of training and by the travelled distance at the last training day. For escape latency, we calculated the summed average time of all trials from the start point to attaining one of the platforms. On the sixth day, the right platform was placed in the opposite quadrant of the maze to confirm that the mice had used spatial cues rather than rule-based learning for navigation. Trials were filmed with a video camera and the swimming trace was extracted using custom-written LabView software (National Instruments).

Water Maze in App^{NL-G-F} mice:

App^{NL-G-F} mice (treated and vehicle) and 14 age- and sex-matched wild-type mice (vehicle) underwent a classical Morris water maze test, which was performed according to a standard protocol with small adjustments (35) as previously described (29). In brief, the first day was used for acclimatization with the platform visible (five minutes per mouse). Then the mice underwent five training days in which each mouse had to perform four trials per day with the

platform visible at the first training day, but submerged on all other training days. The test day consisted of only one trial with complete removal of the platform. The maximum trial length on all training and test days was set to a maximum of 70 seconds. The video tracking software EthoVision® XT (Noldus) was used for analyses of escape latency, the platform visit frequency, and attendance in the platform quadrant at the probe trial.

Immunohistochemistry

Immunohistochemistry in brain regions corresponding to PET analyses was performed for fibrillary as well as oligomeric Aβ, microglia and synaptic density as previously published (36–38). In brief, brains intended for immunohistochemistry were fixed by immersion in 4% paraformaldehyde at 4 °C for 15 hours. Two representative 50 μm thick slices per animal were then cut in the axial plane using a vibratome (VT 1000 S, Leica, Wetzlar, Germany). Free-floating sections were permeabilized with 2% Triton X-100 overnight and blocked with I-Block™ Protein-Based Blocking Reagent (Thermo Fischer Scientific, Waltham, USA). We obtained immunofluorescence labelling of oligomeric Aβ using NAB228 (Thermo Fisher Scientific, USA) with a dilution of 1:500. For histological staining against fibrillar Aβ, we used methoxy-X04 (TOCRIS, Bristol, United Kingdom) at a dilution of 0.01 mg/ml in the same slice as for NAB228 staining. We obtained immunofluorescence labelling of microglia using an Iba-1 antibody (Wako, Richmond, USA) with a dilution of 1:200 co-stained with CD68 (BioRad, California, USA) with a dilution of 1:100. The synaptic density was measured using an anti-vesicular glutamate transporter 1 (VGLUT1) primary antibody (1:500, MerckMillipore). Slices were incubated for 24 hours at 4 °C. After three washes of ten min each in PBS, slices were incubated with an anti-guinea pig Alexa 488 secondary antibody (1:500, Life technologies) for four hours at room temperature. The unbound dye was removed in three washing steps with PBS, and the slices were then mounted on microscope slides with fluorescent mounting medium (Dako, Santa Clara, USA). Images were acquired with a LSM 780 confocal microscope (Zeiss, Oberkochen, Germany) equipped with a 40x/1.4 oil immersion objective. We acquired 3-dimensional 16-bit data stacks of 2048 x 2048 x 120 pixels from five different positions in the frontal cortex at a lateral resolution of 0.17 um/pixel and an axial resolution of 0.4 μm/pixel for Iba1 and CD68 co-staining as well as for NAB228 and methoxy-X04 co-staining. Imaging of VGLUT1 staining was done in a scanned area of $42.43{\times}42.43$ μm^2 with a lateral resolution of 0.083 μm in the CA1-region of the hippocampus. For each mouse, one VGLUT1 image per region was acquired. Images were further processed in Igor Pro to quantify the numbers of single puncta based on morphologic spot detection, as previously described (38). In brief, the sum of the unmixed second partial derivatives in the Cartesian coordinates x and y was calculated from an image and the sum

was then thresholded at a 2×standard deviation of the pixel values to yield a binary image for determining and counting centers of mass for each punctum. Then, the numbers of pre-synapses were normalized to an adjusted image area by subtracting the areas occupied by cell bodies or blood vessels.

Biochemical characterization of brain tissue

DEA (0,2% Diethylamine in 50 mM NaCl, pH 10) and RIPA lysates (20 mM Tris-HCl (pH 7.5), 150 mM NaCl, 1 mM Na2EDTA, 1% NP-40, 1% sodium deoxycholate, 2.5 mM sodium pyrophosphate) were prepared from brain hemispheres. The later was centrifuged at 14,000 g (60 min at 4°C) and the remaining pellet was homogenized in 70% formic acid (FA fraction). The FA fraction was neutralized with 20 x 1 M Tris-HCl buffer at pH 9.5 and used further diluted for Aβ analysis. Aβ contained in FA fractions was quantified by a sandwich immunoassay using the Meso Scale Aβ Triplex plates and Discovery SECTOR Imager 2400 as described previously (39). Samples were measured in triplicates.

Statistics

The principal component of the water maze test was extracted using SPSS 26 statistics (IBM Deutschland GmbH, Ehningen, Germany). Prior to the PCA, the linear relationship of the data was tested by a correlation matrix and items with a correlation coefficient < 0.3 were discarded. The Kaiser-Meyer-Olkin (KMO) measure and Bartlett's test of sphericity were used to test for sampling adequacy and suitability for data reduction. Components with an Eigenvalue > 1.0 were extracted and a varimax rotation was selected. Water maze results were also used as an endpoint in the dedicated manuscript on serial TSPO-PET in both cohorts (23). For immunohistochemistry quantifications GraphPad Prism (Graphpad Prism 7 Software, USA) was used. All analyses were performed by an operator blinded to the experimental conditions. Data were normally distributed according to Shapiro-Wilk or D´Agostino-Pearson test. For assessment of inter-group differences at single time points, Student's t-test (unpaired, two-sided) was applied. All results are presented as mean ± SEM. P values < 0.05 are defined as statistically significant.

3. Results

Long-term pioglitazone treatment provokes a significant increase of the Aβ-PET signal in PS2APP mice

First, we analyzed serial changes of fibrillar amyloidosis under chronic pioglitazone treatment by [^{18}F]florbetaben Aβ-PET in PS2APP mice and wild-type controls. Vehicle treated PS2APP mice showed an elevated Aβ-PET SUVR when compared to vehicle treated wild-type at eight (+20.4%, $p < 0.0001$) and 13 months of age (+37.9%, $p < 0.0001$). As expected, the Aβ-PET SUVR of wild-type mice did not change between eight and 13 months of age (0.831 ± 0.003 vs. 0.827 ± 0.008: $p = 0.645$). Surprisingly, pioglitazone treatment provoked a stronger longitudinal increase in the Aβ-PET signal of PS2APP mice (+21.4%) when compared to vehicle treated PS2APP mice (+14.1%, $p = 0.002$). At the follow-up time point, the Aβ-PET SUVR was significantly elevated when compared to untreated PS2APP mice (Fig. 1; 1.140 ± 0.014 vs.1.187 ± 0.011; $p = 0.0017$). Pioglitazone treatment in wild-type mice provoked no changes of Aβ-PET SUVR compared to vehicle-treated wild-type mice at the follow-up time-point (0.827 ± 0.008 vs. 0.823 ± 0.005: $p = 0.496$). Taken together, we found a significant increase in the Aβ-PET signal, which implied an increase in fibrillary Aβ-levels under pioglitazone treatment in PS2APP mice, wild-type animals showed no changes either with time or in response to pioglitazone treatment.

Figure 1: PPARγ stimulation in PS2APP mice provokes an increase in the Aβ-PET signal. A) Regional analysis of group-averaged standardized uptake value ratio (SUVR) images of the Aβ-PET radiotracer [^{18}F]florbetaben in untreated and in pioglitazone-treated PS2APP mice aged eight and 13 months. Coronal and axial slices are projected upon a standard MRI template. B) Plots show cortical SUVR values of [^{18}F]florbetaben in PS2APP and wild-type (WT) mice between eight and 13 months of age under vehicle (Veh) or pioglitazone (Pio) treatment. The Aβ-PET signal increased in PS2APP mice during aging, but the increase was more pronounced in pioglitazone treated mice ($F_{(1,12)}$ = 12.9; p = 0.0017). In wild-type animals, no difference was observed between untreated and treated animals during aging ($F_{(1,13)}$ = 0.490; p = 0.496). Data are presented as mean ± SEM. P values of Bonferroni *post hoc* test result from two-way ANOVA. N=10-13 PS2APP; N=7-8 WT.

Aβ-PET detects a strong increase of the fibrillar Aβ-load in *App^NL-G-F* mice during chronic PPARγ stimulation

Next, we sought to validate our unexpected findings in PS2APP mice a mouse model with differing Aβ plaque composition, namely the *App^NL-G-F* mouse, which has limited fibrillarity due to endogenous expression of APP with three FAD mutations (25). We thus measured the Aβ-PET signal in *App^NL-G-F* mice during five months treatment with pioglitazone initiated at a baseline age of five months.

Strikingly, the effect of pioglitazone treatment on the Aβ-PET signal was even stronger in *App^NL-G-F* mice than in PS2APP mice. There was a pronounced increase of the Aβ-PET signal during chronic pioglitazone treatment (+17.2%) compared to vehicle (+5.3%, p < 0.0001). *App^NL-G-F* mice with pioglitazone treatment had a higher Aβ-PET SUVR at 7.5 (+4.6%, p = 0.0071) and ten (+7.7%, p < 0.0001) months of age when compared to vehicle-treated *App^NL-G-F* mice (Fig. 2). The baseline level of Aβ-PET SUVR was non-significantly lower in treated compared to untreated *App^NL-G-F* mice (0.878 ± 0.010 vs. 0.906 ± 0.006, p = 0.1350). In both

mouse models, the Aβ-signal increase after pioglitazone-treatment compared to baseline scans was pronounced in the frontotemporal cortex and hippocampal area (Figs. 1A & 2A).

In summary, the pioglitazone treatment augmented the Aβ-PET signal increase in both mouse models; this unexpected result was more pronounced in the *App^{NL-G-F}* model, which expresses less fibrillary Aβ plaques. Furthermore, APP overexpression seemingly did not impact the effects of PPARγ stimulation on the Aβ-PET signal.

Figure 2: Distinct Aβ-PET signal increase upon PPARγ stimulation in *App^{NL-G-F}* mice with limited plaque fibrillarity and without overexpression of APP. A) Regional analysis of group-averaged standardized uptake value ratios (SUVR) of the Aβ-PET radiotracer [^{18}F]florbetaben in untreated and in pioglitazone treated *App^{NL-G-F}* animals at the age of 5, 7.5 and 10 months. Coronal and axial slices are projected upon a standard MRI template. B) Plots show cortical SUVR of [^{18}F]florbetaben in *App^{NL-G-F}* mice between the age of five and ten months under vehicle or pioglitazone treatment. Aβ-PET signal increased in untreated mice during age but the increase was more pronounced in pioglitazone treated *App^{NL-G-F}* mice ($F_{(2,70)}$ = 20.12; p = <0.0001). Data are presented as mean ± SEM. P values of Bonferroni *post hoc* test result from two-way ANOVA. N=14-23.

Pioglitazone triggers a shift towards increased Aβ-plaque fibrillarity in two distinct mouse models of amyloidosis

Given the unexpected *in vivo* findings, we set about to evaluate the molecular correlates of the potentiation of Aβ-PET signal during pioglitazone treatment in AD model mice. More specifically, we investigated whether the signal increase was due to newly formed plaques or a change in plaque composition. To this end, we performed methoxy-X04 staining of fibrillar Aβ as well as NAB228 staining of oligomeric Aβ after PET imaging in *App^{NL-G-F}* (11 months) and PS2APP (14 months) mice. Furthermore, we measured the effect of pioglitazone treatment on the different Aβ-isoforms by ELISA-measurement.

The immunohistochemical analysis showed that the observed increase of the Aβ-PET signal was predominantly explicable by a change in plaque composition rather than by a change in

plaque density (Fig. 3). In both mouse models, the proportion of fibrillary Aβ stained with methoxy-X04 increased significantly under pioglitazone treatment compared to vehicle treated animals (PS2APP: 29.6 ± 3.5% vs. 15.2 ± 0.7%, p = 0.0056, Fig. 3C; App^{NL-G-F}: 9.1 ± 1.6% vs. 4.4 ± 0.4%, p = 0.0001, Fig. 3D). Pioglitazone treatment had no significant effect on the proportion of oligomeric Aβ stained with NAB228 in PS2APP mice (PS2APP: 65.4 ± 6.1% vs. 67.0 ± 6.9%, p = 0.865, Fig. 3C). In App^{NL-G-F} mice, however, the proportion of oligomeric Aβ decreased significantly in treated animals (App^{NL-G-F}: 26.7 ± 1.7% vs. 34.5 ± 1.7%, p = 0.0138, Fig. 3E). The effect size of pioglitazone treatment on plaque morphology was larger in App^{NL-G-F} mice than in PS2APP mice, which was reflected by a significantly increased overlay of methoxy-X04 and NAB228 positive plaques proportions in relation to untreated mice (PS2APP: 40.4 ± 3.6% vs. 25.1 ± 2.1%, p = 0.0075, Fig. 3C; App^{NL-G-F}: 35.0 ± 3.4% vs. 12.9 ± 1.3%, p = 0.0005, Fig. 3E). We attribute this effect to the generally diffuse nature of the plaque composition of App^{NL-G-F} mice, which predominantly contain high oligomeric and low fibrillary fractions of Aβ (40) (compare Fig. 3A and Fig. 3B).

The number of methoxy positive Aβ-plaques were similar between vehicle and pioglitazone treated groups for PS2APP (1016 ± 107 vs. 1118 ± 121, p = 0.547, Fig. 3D) and App^{NL-G-F} mice (242 ± 56 vs. 266 ± 33, p = 0.722, Fig. 3F). Notably there was no significant effect of chronic pioglitazone treatment on the different insoluble Aβ species (Aβ40, Aβ42) as well as on the level of the soluble Aβ42-isoform observed in either mouse model (Suppl. Fig. 1A). Taken together, our results indicate that the potentiated increase of the Aβ-PET signal upon pioglitazone treatment reflected a change in plaque composition from oligomeric to fibrillary Aβ-fractions. The change was not detectable by biochemical analysis.

Figure 3: Pioglitazone treatment triggers a change in plaque composition in two different mouse models of amyloidosis. Staining of fibrillary Aβ (methoxy-X04, cyan) and oligomeric Aβ (NAB228, magenta) in vehicle and pioglitazone treated PS2APP mice A) and App^{NL-G-F} mice B). C) The plaque area covered by methoxy-X04 staining was significantly higher ($t_{(9)}$ = 3.612; p = 0.0056), whereas the plaque area covered by NAB228 staining remained equal ($t_{(10)}$ = 0.175; p = 0.865) in pioglitazone treated PS2APP mice. The overlay of

NAB228 and methoxy staining increased under pioglitazone treatment ($t_{(9)}$ = 3.432; p = 0.0075). D) The number of methoxy positive Aβ-plaques did not change under pioglitazone treatment in PS2APP-mice. E) In App^{NL-G-F} mice, methoxy coverage ($t_{(11)}$ = 5.802; p = 0.0001), NAB228 coverage ($t_{(11)}$ = 5.80; p = 0.0001), as well as the overlay of both stainings ($t_{(11)}$ = 2.93; p = 0.0138), increased under pioglitazone treatment. F) In App^{NL-G-F} mice, the number of methoxy positive Aβ-plaques did not change under pioglitazone. Data are presented as mean ± SEM; n = 5-13 mice. Two-sample student´s t-test results: * p < 0.05; ** p < 0.01; *** p < 0.001.

Microglial activation is reduced upon PPARγ stimulation in both AD mouse models

Furthermore, we aimed to confirm whether the previously reported shift of the microglial activation state towards more inactive gene expression patterns upon pioglitazone treatment (15; 14) was also present in both mouse models. To detect changes in the activation state of microglial cells, we performed Iba1 as well as CD68 immunohistochemical staining of activated microglia in both mouse models. We observed that pioglitazone treatment significantly decreased microglial activation in both mouse models (Fig. 4). In PS2APP mice, PPARγ stimulation provoked a one-third reduction of area coverage of Iba1-positive microglial cells (area: 9.1 ± 0.6%) compared to untreated mice (14.0 ± 0.5%, p = 0.0003), and also a significant reduction of CD68-positive microglial cells area (7.6 ± 0.4% vs. 9.9 ± 0.3%, p = 0.0018). In pioglitazone treated App^{NL-G-F} mice, the area reduction was less pronounced, but still significant for Iba1-positive microglial cells (9.4 ± 0.2% vs. 10.6 ± 0.2%, p = 0.0015) and CD68-positive microglial cells (2.7 ± 0.1% vs. 3.0 ± 0.1%, p = 0.0141) compared to untreated mice. Thus, we observed a consistent net reduction of activated microglial coverage in both models; the lesser effect in App^{NL-G-F} mice might indicate partial compensation by triggering of microglial activation due to increased fibrillary Aβ levels (40).

Figure 4: Pioglitazone treatment reduces microglial activation in both AD mouse models. Iba1- (magenta) as well as CD68-(cyan) positive microglial cells in PS2APP A) and App^{NL-G-F} mice B). C) The area of Iba1 positive microglial cells ($t_{(8)}$ = 5.95; p = 0.0003) as well as CD68 positive microglial cells ($t_{(8)}$ = 4.58; p = 0.0018) decreased in treated PS2APP mice. The same effect was observed in App^{NL-G-F} mice were the area covered by Iba1 positive ($t_{(11)}$ = 4.21; p = 0.0015) as well as CD68 positive microglial cells ($t_{(11)}$ = 2.91; p = 0.014) were significantly reduced in treated compared to untreated mice. Data are presented as mean ± SEM; n = 5-7 mice. Two-sample student´s t-test results: * p < 0.05; ** p < 0.01; *** p < 0.001.

Cognitive function is improved by chronic pioglitazone treatment in association with an increasing Aβ-PET rate of change

Finally, we aimed to elucidate whether the observed longitudinal changes in the composition of Aβ-plaques affected synaptic density and hippocampus related cognitive performance. To this end we performed assessment of spatial learning by water maze testing and glutamate transporter staining as a read-out of synaptic density. In order to increase the robustness of spatial learning parameters in a correlation analyses, we performed a principal component analysis of the behavioral readouts, and used the principal component as a condensed index of spatial learning performance in individual mice.

In PS2APP mice, treatment with pioglitazone resulted in a significant reduction of the distance travelled compared to untreated mice during the probe trial (Fig. 5A; distance: 154 ± 17 pixels vs. 309 ± 65 pixels, p = 0.0156), whereas in wild-type animals there was no difference between treated and untreated animals (distance: 110 ± 10 pixels vs. 71 ± 14 pixels, p = 1.00). The performance in water maze (principal component) of pioglitazone treated PS2APP mice correlated strongly with the rate of increase in Aβ-PET signal (Fig. 5C; R^2 = 0.470; p = 0.0097). In App^{NL-G-F} mice, pioglitazone treatment did not result in a significant change of spatial learning performance (Fig. 5B; escape latency: 21.4 ± 3.0 s vs. 20.1 ± 3.7 s, p = 0.7706). Accordingly, the performance in water maze (principal component) and the rate of change in the Aβ-PET signal of pioglitazone treated App^{NL-G-F} mice did not correlate (Fig. 5D; R^2 = 0.0022; p = 0.878).

To explore the basis of water maze results in PS2APP mice at the molecular level, we performed staining of synaptic density in the hippocampus. In AD, excessive concentrations of Aβ reduces synaptic plasticity, which ultimately leads to their degeneration and even neuronal death (41–43) . However, Aβ-oligomers are the primary neurotoxic forms of Aβ, while Aβ-fibrils have less neurotoxicity (44–46). Thus, we hypothesized that pre-synaptic density in the hippocampal CA1-Area, as assessed by the anti-vesicular glutamate transporter 1 (VGLUT1) primary antibody, would be rescued in pioglitazone-treated PS2APP mice compared to untreated controls (Fig. 5E). In wild-type mice we did not observe altered changed VGLUT1 density under pioglitazone treatment (Fig. 5F; 0.519 ± 0.007 1/µm vs.

0.502 ± 0.008 1/µm, p = 0.270). In PS2APP mice, however, we found that pioglitazone treatment significantly rescued spine density in the CA1-region of the hippocampus compared to untreated animals (Fig. 5F; 0.497 ± 0.006 1/µm vs. 0.459 ± 0.007 1/µm, p = 0.0004), supporting the hippocampal-dependent water maze results.

Figure 5. Improved spatial learning correlates with an increased Aβ-PET rate of change in PS2APP mice. A) Pioglitazone treated PS2APP mice achieved a shorter travel distance in the water maze test compared to untreated PS2APP mice ($F_{(3,34)}$ = 7.663; p = 0.0156; N=10-13), whereas wild-type animals showed no significant difference ($F_{(3,34)}$ = 0.66; p = 1.00; N=7-8). B) Treated App^{NL-G-F} mice showed no difference in escape latency compared to untreated animals ($t_{(33)}$ = 0.294; *p* = 0.771; N=14-21). C) Scatter plots show correlations between the Aβ-PET rate of change ([^{18}F]florbetaben; ΔSUVR) during the treatment period and individual cognitive testing scores (principal component analysis) in PS2APP mice and D) in App^{NL-G-F} mice (R indicates Pearson's coefficient of correlation) E) VGLUT1 staining in the hippocampal CA1-region of representative untreated and treated wild-type (WT) mice (upper row) as well as of representative untreated and treated PS2APP mice. F) The decrease in synaptic density in the hippocampal CA1-region as assessed by VGLUT1 staining was ameliorated in treated PS2APP mice when compared to untreated mice, whereas no such treatment effect was seen in wild-type animals ($F_{(3,34)}$ = 12.03; p = <0.0001; N=7-13). Bonferroni *post hoc* test results of one-way ANOVA (A,F) and two-sample student´s *t*-test results (B): * p < 0.05; *** p < 0.001. Data are presented as mean ± SEM.

4. Discussion

To our knowledge, this is the first large-scale longitudinal PET study of cerebral Aβ-deposition in two distinct AD mouse models treated with the PPARγ agonist pioglitazone. In this study, we combined *in vivo* PET monitoring with behavioral testing and detailed immunohistochemical analysis. Our main finding was an unexpected potentiation in both mouse models of the increasing Aβ-PET signal during five months of pioglitazone treatment. This increase occurred despite an improvement of spatial learning and prevention of synaptic loss in the treated mice. Immunohistochemistry revealed a shift towards plaque composition of higher fibrillarity as the molecular correlate of the Aβ-PET signal, which was directly associated with improved cognitive performance in PS2APP mice.

Aβ-PET enables longitudinal *in vivo* detection of Aβ-plaques, which plays an important role in AD diagnosis, monitoring disease progression, and as an endpoint for therapeutic treatment effects (47). In our preceding observational and interventional studies, we validated in AD model mice the clinically established Aβ-PET tracer [18F]florbetaben relative to histologically defined indices Aβ deposition (3; 21). So far, an enhanced or increasing [18F]florbetaben-PET signal has been interpreted as an indicator of disease progression or treatment failure (48). Unexpectedly, we found that pioglitazone potentiated the increasing Aβ-PET signal in two mouse models compared to vehicle controls; in both cases, this increase was due to a shift of the plaque composition towards higher fibrillarity, and away from the more neurotoxic oliogomeric form. In particular, our immunohistochemical staining study revealed a shift from oligomeric to a more fibrillary Aβ-fractions with pioglitazone treatment. However, ELISA measurements of plaque associated fibrillary Aβ extracted with formic acid did not indicate a change in the Aβ species composition in brain. This suggests that Aβ-PET imaging and immunohistochemical analysis detect treatment effects on Aβ-plaque composition that do not arise from a shift in the levels of Aβ species, and which may thus evade detection in studies of CSF or plasma content (49).

Furthermore, our study provides evidence that rescued spatial learning deficits and prevented hippocampal synaptic loss can occur despite an increasing Aβ-PET signal upon immunomodulation. The combined results might sound contradictory, but according to the amyloid cascade hypothesis, Aβ-oligomers rather than Aβ-fibrils are the neurotoxic Aβ-forms (44; 50). Indeed, high concentrations of Aβ-oligomers isolated from brain of AD patients correlated significantly with the degree of cognitive impairment prior to death (51–53). Furthermore, Aβ-oligomers have been shown to disrupt long-term potentiation at synapses and provoke long-term depression (54–56). The binding of Aβ-oligomers to synapses

additionally triggers a variety of aberrant signaling pathways and thereby alters synaptic plasticity and transmission, ultimately resulting in an impairment of cognitive functions (57; 58; 46). Thus, improved spatial learning and rescued synaptic density could reflect a therapeutically induced shift of Aβ to hypercondensed plaques, in keeping with observations of greater neuritic damage in association with more diffuse plaques (59; 60). Furthermore, strongly in line with our present translational data, a recent study argued that dense-core plaques may play a protective role in AD (61). In that study, microglia promoted the formation of dense-core plaques, which promoted the removal of toxic Aβ-oligomers from the vicinity of neurons (61).

The shift in plaque composition was more pronounced in App^{NL-G-F} mice than in the PS2APP model. Due to the expression of the Arctic mutation (25), the Aβ-deposits of the App^{NL-G-F} line consist predominantly of Aβ-oligomers (29; 40). The plaques formed in App^{NL-G-F} mice have a composition resembling that of Aβ-deposits found in patients an early stage of AD (62; 63). However, we observed no improvement in cognition in the APP knock-in mouse line after pioglitazone treatment. We attribute the lacking improvement of spatial learning to the minor deterioration of this model in water maze assessment at ten months of age (64; 29). A beneficial effect of pioglitazone on spatial learning might be observed if pioglitazone would be administered at a later stage in the App^{NL-G-F} mouse model manifesting in more severe cognitive impairment. Our present observation stand in contrast with previous studies showing that PPAR-γ agonists reduced Aβ-plaque formation by increasing Aβ-clearance (15; 65; 14). However, those studies only performed endpoint analyses, in part after short-term treatment of nine days (14); the current work is the first to perform longitudinal *in vivo* monitoring of Aβ-deposition over a five-month chronic PPAR-γ treatment period. We note that the divergent results could also reflect the different markers used for immunohistochemistry compared to our present differentiated analysis of fibrillar and oligomeric Aβ components. As such, the decreased NAB228-positive plaque fraction in our treated App^{NL-G-F} mice fits to the earlier reported decrease of the 6E10-positive area in APPPS1 mice (14). Furthermore, our preclinical study indicates, that the [^{18}F]florbetaben-PET signal primarily represents more condensed fibrillary Aβ-plaques, which are linked to amelioration of spatial memory impairments. Therefore, increases in the [^{18}F]florbetaben-PET signal must be precisely differentiated and interpreted with caution. We note that the biochemical source of the Aβ-PET signal is still a matter of controversy, since some studies found no impact of non-fibrillar plaque components (66) whereas others postulated a significant contribution of non-fibrillar Aβ to the Aβ-PET signal (67–69). Recently, we were able to show that non-fibrillar components of Aβ plaques indeed contribute to the net Aβ-PET signal (70). Development of new PET tracers that selectively target oligomeric Aβ may realize a more precise discrimination of neurotoxic Aβ plaque manifestation (71; 72) and its

impact on disease severity.

In line with previous pioglitazone studies (14; 15), we observed a decrease in microglial activity (23), thus confirming the immunomodulatory effect of the drug. In the parallel work, we called into question the net microglial activation level after chronic PPARγ stimulation, since earlier studies have shown that fibrillary Aβ-deposits activate microglial cells (40) which then migrate towards the fibrillar deposits (6), resulting in an increased number of activated microglial cells surrounding Aβ-plaques (8). Hence, the inactivation and migration effects could cancel each other out. Based on our findings in both AD models, we conclude that, by increasing plaque fibrillarity, the immunomodulatory effect of pioglitazone overweighs the potential triggering of activated microglia. Emerging interest in the immunological processes in the pathophysiology of AD is drawing attention to new therapeutic targets besides purely symptomatic treatments (acetylcholinesterase inhibitors and NMDA receptor antagonists) and anti-amyloid interventions (73). Modulating microglial phenotype to restore their salutogenic effects may prove crucial in new therapeutic trials (74). In response to Aβ-deposition, microglial cells normally undergo an inflammatory activation, leading to a proinflammatory milieu that interferes with synapse maintenance and the clearance of Aβ deposits from brain (14; 4).

In several preclinical and clinical trials, pioglitazone proved to be a promising immunomodulatory approach for treatment of AD, especially in patients with comorbid diabetes (75; 76). However, preclinical data also showed divergent effects of PPARγ treatment on microgliosis and amyloidosis (77), and a meta-analysis of clinical trials did not indicate a significantly beneficial effect of PPAR-γ agonists on memory in patients with mild-to-moderate AD (18). Furthermore, a phase III trial of pioglitazone in patients with mild AD was discontinued due to lacking efficacy (19). Our data calls for monitoring of the effects of PPARγ agonists by Aβ-PET, which may help to stratify treatment responders based on their individual rates of Aβ plaque accumulation. Based on our results, we submit that personalized PPARγ agonist treatment might be effective when the patient has capacity to successfully shift toxic oligomeric Aβ towards fibrillar parts of the plaque.

In conclusion, chronic pioglitazone treatment provoked a longitudinal Aβ-PET signal increase in transgenic and knock-in mice due to a shift towards hypercondensed fibrillar Aβ plaques. The increasing rate of Aβ-PET signal increase with time was accompanied by ameliorated cognitive performance and attenuated synaptic loss after pioglitazone treatment. It follows that increasing Aβ-PET signal need not always indicate a treatment failure, since it is the composition of Aβ plaques that determines their neurotoxiticy. In summary, our preclinical data indicate that a shift towards increasing fibrillar amyloidosis can be beneficial for the preservation of cognitive function and synaptic integrity.

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6. Disclosures

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8. Supplement

Supplemental figure 1. Insoluble Aβ species as well as soluble Aβ42 did not change upon pioglitazone treatment in both mouse models. A) ELISA-measurements showed a trend to reduced insoluble Aβ-isoform levels under pioglitazone treatment in PS2APP mice but did not reach significance for the different Aβ fractions. PS2APP vehicle controls indicated 882.7 (± 109.7) pg/ml Aβ40 and pioglitazone treated PS2APP mice indicated 664.2 (± 90.7) pg/ml Aβ40 (p = 0.496; N=10; two-sample student´s t-test). PS2APP vehicle controls indicated 4309.4 (± 26.6) pg/ml Aβ42 and pioglitazone treated PS2APP mice indicated 4250.0 (± 162.8) pg/ml Aβ42 (p = 0.456; N=10; two-sample student´s t-test). Levels of soluble Aβ42 did also not significantly change upon PPARγ-treatment in PS2APP mice. PS2APP vehicle controls indicated 1265.3 (± 190.1) pg/ml soluble Aβ42 and pioglitazone treated PS2APP mice indicated 1116.5 (± 161.9) pg/ml soluble Aβ42 (p = 0.559, N=10; two-sample student´s t-test). B) No significant change in the levels of insoluble Aβ-isoforms was observed upon PPARγ stimulation in App[NL-G-F] mice. Vehicle control App[NL-G-F] mice indicated 498.8 (± 93.0) pg/ml Aβ40 and pioglitazone treated App[NL-G-F] mice indicated 466.0 (± 95.1) pg/ml Aβ40 (p = 0.496, N=9). Vehicle control App[NL-G-F] mice indicated 3901.8 (± 245.8) pg/ml Aβ42 and pioglitazone treated App[NL-G-F] mice indicated 3650.1 (± 471.0) pg/ml Aβ42 (p = 0.198; N=9; two-sample student´s t-test). No significant increase in the levels of soluble Aβ42 was observed upon PPARγ stimulation in *App[NL-G-F]* mice. App[NL-G-F] vehicle controls indicated 12.1 (± 5.2) pg/ml soluble Aβ42 and pioglitazone treated App[NL-G-F] mice indicated 11.4 (± 5.1) pg/ml soluble Aβ42 (p = 0.789, N=9; two-sample student´s t-test).

A

	Vehicle		Pioglitazone	
	8.0 M	13.0 M	8.0 M	13.0 M

0.8 ——————— 1.4

SUVR$_{WM}$

B

Aβ-PET (SUVR$_{CTX/WM}$)

1.30

1.10

0.90

0.70

8M 13M   8M 13M   8M 13M   8M 13M

PS2APP Veh   PS2APP Pio   WT Veh   WT Pio

A

	Iba1	CD68	Merge

PS2APP — Vehicle, Pioglitazone

B

App^NL-G-F — Vehicle, Pioglitazone

20 μm

C

● PS2APP vehicle   ● PS2APP pioglitazone   ▲ *App^NL-G-F* vehicle   ▲ *App^NL-G-F* pioglitazone

[%] Area covered Iba1   ***

[%] Area covered CD68   **

[%] Area covered Iba1   ****

[%] Area covered CD68   *