1	Title:
2	A studyforrest extension, MEG recordings while watching the audio-visual movie
3	"Forrest Gump"
4	
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21	

22 Abstract

Naturalistic stimuli, such as movies, are being increasingly used to map brain 23 function because of their high ecological validity. The pioneering studyforrest and 24 other naturalistic neuroimaging projects have provided free access to multiple movie-25 watching functional magnetic resonance imaging (fMRI) datasets to prompt the 26 community for naturalistic experimental paradigms. However, sluggish blood-27 oxygenation-level-dependent fMRI signals are incapable of resolving neuronal 28 activity with the temporal resolution at which it unfolds. Instead, 29 30 magnetoencephalography (MEG) measures changes in the magnetic field produced by neuronal activity and is able to capture rich dynamics of the brain at the millisecond 31 32 level while watching naturalistic movies. Herein, we present the first public prolonged MEG dataset collected from 11 participants while watching the 2 h long audio-visual 33 34 movie "Forrest Gump". Minimally preprocessed data was also provided to facilitate the use. As a studyforrest extension, we envision that this dataset, together with fMRI 35 36 data from the *studyforrest* project, will serve as a foundation for exploring the neural dynamics of various cognitive functions in real-world contexts. 37

39 Background & Summary

The mechanisms of human brain function in complex dynamic environments is 40 the ultimate mystery that cognitive neuroscience aspires to quest. Most of the existing 41 models on brain function have been obtained from tightly controlled experimental 42 manipulations on carefully designed "artificial" stimuli. However, these simple 43 stimuli are often irrelevant to ecological scenarios encountered in real-world 44 environments, in terms of quantity, complexity, modality, and dynamics. To address 45 this issue, naturalistic stimuli that encode a wealth of real-life content have become 46 increasingly popular for understanding brain function in ecological contexts. 47 Researchers have achieved significant advances in the areas of human memory, 48 49 attention, language, emotions, and social cognition using naturalistic stimuli (for recent reviews, please refer to Sonkusare et al., 2019¹ and Jääskeläinen et al., 2021²). 50 Simultaneously, emerging deep learning technologies that could afford multiple levels 51 of representations for naturalistic stimuli are continuously expanding the application 52 of naturalistic stimuli for exploring human brain function $^{3-6}$. 53

Notably, owing to its dynamics and multimodal content, movies have been 54 55 successfully utilized as naturalistic stimuli to examine the mechanism by which the brain processes diverse psychological constructs and dynamic interactions. Functional 56 magnetic resonance imaging (fMRI) is commonly employed to measure brain activity 57 while watching a movie. In particular, the pioneering studyforrest and other 58 naturalistic neuroimaging projects have released multiple fMRI datasets collected 59 from participants who watched movie clips^{7–11}. However, fMRI measures the 60 relatively sluggish blood-oxygenation-level-dependent signal, therefore falling short 61 of characterizing the complex neural dynamics underlying the cognitive processing of 62 dynamic movies. In contrast, magnetoencephalography (MEG) measures the magnetic 63 fields generated by neuronal activity on a millisecond time scale. Thus, it has great 64 potential to pry open neural dynamics in processing naturalistic stimuli. Several 65 66 studies have leveraged MEG to investigate brain activity for naturalistic movie stimuli in a short period ($\leq 20 \text{ min}$)^{12–16}. So far, however, there is still a dearth of publicly 67 accessible MEG recordings for naturalistic stimuli, especially prolonged MEG 68 recordings for dynamic movies that are more likely to capture the 69 temporal dynamics of regular functional brain states that occur in everyday life, and 70 further contribute to unraveling human brain function in ecological contexts. 71

72 Herein, we present an MEG dataset obtained while watching the 2 h long 73 audio-visual movie "Forrest Gump" (R. Zemeckis, Paramount Pictures, 1994). The 74 recordings measure brain activation with a temporal resolution at the millisecond level, thus providing a timely and efficient extension to the *studyforrest* dataset. 75 76 Specifically, MEG data were collected from 11 participants while they were watching the Chinese-dubbed movie "Forrest Gump" in eight consecutive runs, each lasting for 77 roughly 15 min. High-resolution structural MRI was additionally acquired for all 78 participants, thereby allowing the incorporation of the detailed anatomy of the brain 79 and head in the source localization of MEG signals. Together with the raw data, 80 preprocessed MEG and MRI data with standard pipelines were also provided to 81 82 facilitate the use of the data. Considering MEG and fMRI are complementary to each other, synergy between our present MEG recordings and fMRI data from the 83 studyforrest project will serve as a front to elaborate brain function in the wild. We 84 believe the dataset is suitable for addressing many questions pertaining to the neural 85 dynamics of various aspects, including perception, memory, language, and social 86 87 cognition.

88 Methods

89 Participants

A total of 11 participants (mean \pm SD age: 22 \pm 1.7 years, 6 female) from the 90 Beijing Normal University, Beijing, China, volunteered for this study. They 91 completed both the MEG and MRI sessions. All participants were right-handed native 92 93 Chinese speakers, with normal hearing and normal or corrected-to-normal vision. None of them had ever watched the film "Forrest Gump" before, except one who had 94 95 watched some clips, however not the entire movie. Of the 10 participants, four had heard about the movie plot, while others did not. The study was approved by the 96 97 Institutional Review Board of the Faculty of Psychology, Beijing Normal University. 98 Written informed consent was obtained from all participants, prior to their 99 participation. All participants provided additional consent for sharing their anonymized data for research purposes. 100

101 **Procedures**

Fig. 1 depicts the overall flow of data collection and preprocessing. Prior todata acquisition, all participants completed a questionnaire on their demographic

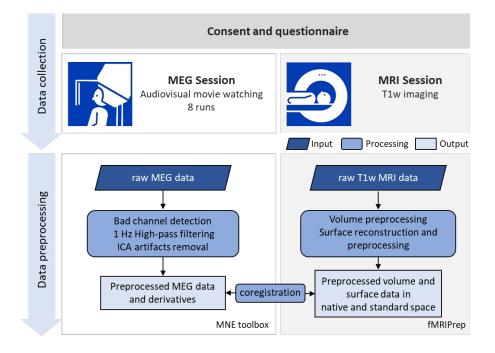
104 information and familiarity with the movie "Forrest Gump". The data acquisition

105 consisted of two sessions for each participant, namely one MEG session to record

their neural activities during movie watching and an MRI session with a T1-weighted

107 (T1w) scan to measure the brain structure for the spatial localization of the MEG

- signal. The MRI scan immediately followed the MEG session for all participants,
- 109 except for sub-07 and sub-11, who finished their MRI session a week later.
- 110



111

112 Fig. 1. Schematic of the data collection and preprocessing procedure. Data

collection comprised one MEG session, followed by one MRI session. The

neuromagnetic signals were recorded with a whole-scalp-covering MEG while the

115 participants watched the audio-visual movie "Forrest Gump". An anatomical T1w

imaging was acquired in the MRI session. The raw MEG data and MRI data were

117 preprocessed with MNE and fMRIPrep toolbox, respectively. The MEG-MRI

118 coregistration was performed on the preprocessed data.

119 Stimulus material and presentation

The audio-visual stimuli were generated from the Chinese-dubbed "Forrest
Gump" DVD, released in 2013 (ISBN: 978-7-7991-3934-0). The movie was split into
eight segments, each of which lasted for approximately 15 min. The stimuli were
initially obtained by concatenating all original VOB files from the DVD release into
one MPEG-4 file, using FFmpeg (https://ffmpeg.org). The concatenated MPEG-4 file
contained a video stream and a Chinese-dubbed audio stream, which was down-mixed

126 from multi-channel to 2Channel stereo. The stimuli were then divided into eight

segments using Adobe Premier software (Adobe Premiere Pro CC 2017, Adobe, Inc.,

- 128 San Jose, CA, USA). Each segment conformed to the following specifications: video
- 129 codec=avc1, display aspect ratio=4:3, resolution=1024×768 pixels, frame rate=25
- 130 FPS, color space=YUV, video bit depth=8 bits, audio codec=mp4a-40-2, audio
- sampling rate=48.0 kHz, and audio channels=2. Each successive segment began with
- a 4 s repetition of the end of the previous segment. It should be noted that the Chinese-
- 133 dubbed "Forrest Gump" was slightly abridged than the German version. To align with
- the stimuli of the *studyforrest* dataset as much as possible, a short clip from the
- 135 German-dubbed DVD released in 2011 (EAN: 4010884250916) was added to our
- 136 stimuli. Table 1 summarizes the alignment of the stimuli sources from both the
- 137 Chinese and German versions.
- 138

Segment	Frames	Duration	Start (cn)	End (cn)	Start (de)	End (de)
1	22499	15:00.07	63	22562	35	22534
2	22500	45.04.00	22463	32374	22438	32349
2	22599	15:04.08	36410	49098	36385	49073
			48999	57860	48974	57835
2	22500	15.04.00	58531	63717	58506	63692
3	22599	15:04.08	-	-	63692	64621
			63718	71341	64621	72244
			71242	85132	72146	86036
4	22599	15:04.08	00407	97136	89332	93902
			88427	97136	94464	98603
			07027	111710	98504	105793
5	22500	15.04.00	97037	111719	109959	117352
5	22599	15:04.08	115101	118317	120733	123949
			118797	123498	125347	130048
C	22500	15.04.08	123398	145602	129948	152152
6	22599	15:04.08	147736	148131	154286	154681
7	22599	15:04.08	148032	170631	154582	177181
8	17661	11:46.56	170532	188193	177082	194743

139

Table 1. Timing alignment for stimuli from the Chinese (cn) and German (de)
version of "Forrest Gump". The start time and end time are different for the same
movie clip in the two versions. Moreover, a clip with only background sound stream
from the German version (frames from 63692 to 64621) was added into the third
segment.

145

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    The visual stimuli were projected onto a screen in full-screen mode from a
    DLP projector with 1024×768-pixel resolution, using Psychophysics Toolbox Version
    3<sup>17</sup> in MATLAB 2016 (The MathWorks, Inc., Natick, Massachusetts, USA). The
    participants watched the visual stimuli on a rear projection screen through mirror
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reflection (visual field angles=31.17°×23.69°; viewing distance=751 mm). The audio

stimuli were delivered to the participants using foam ear-tips connected to a

152 loudspeaker via an air-conducting tube. The average delay of the peripheral devices

153 was 33 ms and 15 ms for the visual and audio displays, respectively. The participants

154 were instructed to watch the movie, without other tasks and keep still as best as

155 possible.

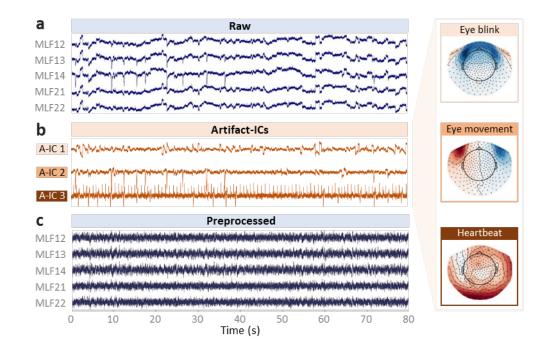
156 MEG data acquisition

157 MEG data were recorded using a 275-channel whole-head axial gradiometer DSQ-3500 MEG system (CTF MEG, Canada) at the Institute of Biophysics, Chinese 158 159 Academy of Sciences, Beijing, China. Three channels (i.e., MLF55, MRT23 and MRT16) were out of service due to failure of sensors. The neuromagnetic signals were 160 recorded in continuous mode at a sampling rate of 600 Hz, without online digital band 161 filters. A third-order synthetic gradiometer was employed to remove far-field noise. 162 The precise timing of each frame was recorded. Upon presenting each frame to the 163 participants, we recorded a trigger pulse lasting for five samples in the stimuli channel 164 UPPT001, along with the MEG signals. The beginning of the movie was indicated 165 with a value of 255. Owing to the limited bit-width of the stimuli channel, the frame 166 number was unable to be marked with an accurate value > 20,000. The frame numbers 167 were therefore marked as the ceiling of the timestamp of that frame divided by 10, 168 resulting in step-like increasing marker values with a step width of 10 s. 169

170 At the beginning of each session, three HPI coils were attached to the participants' nasion (NAS), left preauricular (LPA), and right preauricular (RPA) 171 172 points to continuously measure their head position during the MEG dewar. A customized wooden chin-rest supporter was introduced to prevent possible head 173 174 movements. The MEG session consisted of eight runs, with each run playing one 175 movie segment. Eight segments were played chronologically. The participants took a 176 self-paced break between runs. Following the completion of the MEG scan, the participants underwent an anatomical T1w scan. The HPI coils were replaced with 177 three customized MRI-compatible vitamin E caplets in the MRI scan to provide 178 spatial reference for the spatial alignment between the MEG and MRI data. 179

181 MEG data preprocessing

MEG data processing was performed offline using the MNE-Python 182 package¹⁸. The MEG preprocessing pipeline was conducted at the run level (Fig. 1). 183 First, the bad channels were detected and marked. As a result, no bad channels were 184 identified in all acquisitions except two in run-05 of sub-05. Second, a high-pass filter 185 of 1 Hz was applied to remove possible slow drifts from the continuous MEG data 186 (Fig. 2a). Finally, artifact removal was performed using an independent component 187 analysis (ICA). The number of independent components (IC) was set to 20. Two raters 188 (i.e., X.L. and Y.D.) manually identified the head movement, eye movement, eye 189 blinks, and cardiac artifacts (Fig. 2b). On average, 3.21 ICs (SD: 0.85) were classified 190 as artifacts. The denoised MEG data were eventually reconstructed from all the non-191 artifact components and residual components (Fig. 2c). Both the raw and preprocessed 192 193 data were provided in the released dataset. 194



196 Fig. 2. Typical artifact-ICs and MEG signals from the pre- and post-

- 197 preprocessing data. (a) MEG signals of example channels from the raw (i.e. pre-
- 198 preprocessing) data. (b) Timeseries and scalp field distribution of three typical
- artifact-ICs (A-ICs), namely A-IC 1 for eye blink, A-IC 2 for horizontal eye
- 200 movement, and A-IC 3 for heartbeat. (c) MEG signals of example channels from the
- 201 preprocessed data. Data from the run-04 of sub-04 was used for this illustration.

202 MRI data acquisition and preprocessing

High-resolution anatomical MRI was collected for each participant using a 3T 203 SIEMENS Prisma^{fit} scanner (Siemens Healthcare GmbH, Erlangen, Germany), with a 204 20-channel headneck coil. All participants underwent a T1w scan with a 3-D 205 magnetization-prepared rapid gradient-echo pulse sequence with identical parameters 206 (TR=2530 ms, TE=1.26 ms, TI=1100 ms, flip-angle=7°, 176 sagittal slices, slice 207 thickness=1 mm, matrix size= 256×256 , and voxel size= 1.0×1.0 mm), except that 208 209 sub-01 was scanned with slightly different parameters (TR=2200 ms, TE=3.37 ms, TI=1100 ms, flip-angle=7°, 192 sagittal slices, slice thickness=1 mm, matrix 210 size= 224×256 , and voxel size= 1.0×1.0 mm). Earplugs were used to attenuate the 211 scanner noise. A foam pillow and extendable padded head clamps were applied to 212 restrain the head motion. 213 The raw DICOM files of T1w images to NIFTI files using dcm2niix 214 (https://github.com/rordenlab/dcm2niix). The T1w images were then minimally 215 preprocessed using the anatomical preprocessing pipeline from fMRIPrep 20.2.1, with 216 default settings¹⁹. In brief, the T1w data were skull-stripped and corrected for intensity 217 nonuniformity with ANTs and N4ITK²⁰. Brain surfaces were reconstructed using 218

219 FreeSurfer²¹. Spatial normalization to both MNI152NLin6Asym and

220 MNI152NLin2009cAsym was performed through nonlinear registration with ANTs,

using the brain-extracted versions of both T1w volume and template.

222 MEG-MRI coregistration procedure

To reconstruct the source of MEG sensor signals, MEG data were co-223 224 registered with the high-resolution anatomical T1w MRI data for each participant. The NAS, LPA, and RPA points marked in both MEG and MRI sessions were used as 225 fiducial points for the alignment of the MEG and MRI data. Specifically, following 226 the generation of a high-resolution head surface using MNE make scalp surfaces 227 based on FreeSurfer reconstruction, we performed MEG-MRI coregistration for each 228 participant in the MNE COREG GUI¹⁸. First, the three fiducial points were manually 229 pinned on the MRI-reconstructed head surface. an iterative algorithm (nearest-230 neighbor calculations) was then ran to align the MEG and MRI coordinates. The co-231 registration was refined by manual adjustment. The results showed that the averaged 232 233 distances between the three fiducials in the coregistered MEG and MRI coordinate systems were 0.96 mm, 4.22 mm, and 4.90 mm for NAS, LPA, and RPA respectively. 234

Both the MRI-fiducials files and MEG-MRI coordinate transformation files were

236 included in the released data.

237 Data Records

238The dataset can be accessed at OpenNeuro (dataset accession number:

ds003633, version 1.0.1, https://openneuro.org/datasets/ds003633/versions/1.0.1)²².

240 The facial information was removed from the published dataset using pydeface

241 (https://github.com/poldracklab/pydeface) to ensure anonymity. The data was

organized according to the MEG-Brain Imaging Data Structure (MEG-BIDS)²³ using

243 the MNE-BIDS toolbox 24 (Fig. 3). Besides dataset and participant description files,

the data were sorted into different directories, including "sub-<participant_id>,"

- 245 "derivatives," and "code" directory for raw data from each participant, preprocessed
- 246 data, and the code used for stimuli preparation and presentation, data preprocessing,

247 respectively (Fig. 3a).

248



Fig. 3. The file structure of the dataset. (a) File structure of the project directory. **(b)**

- File structure of the raw data for each individual participant. (c) File organization of the derived (preprocessed) data
- the derived (preprocessed) data.
- 253

254 Raw data

The raw data of each participant were stored separately in the "sub-255 <participant id>" folders (Fig. 3b), consisting of two subfolders, namely "anat" and 256 "meg". The T1w MRI data ("*T1w.nii.gz") and associated sidecar json files were 257 located in the "anat" folders. The raw MEG data were provided as CTF ds files 258 ("* meg.ds") for each run, and located in the "meg" folder along with sidecar json 259 files. In addition, "* channel.tsv" files with MEG channel information, "* events.tsv" 260 files with the presentation timing of stimuli frames and "*coordsystem.json" files with 261 262 coordinate system information of the MEG sensors were included in the "meg" folder. In parallel with the "sub-<participant id>" directories, a "sub-emptyroom" 263 264 directory hosted empty-room MEG measurements, which recorded the environmental noise of the MEG system. The empty-room measurements lasted for 34 s and were 265

acquired on each data acquisition day, except for the day 20190603.

267 Preprocessed data

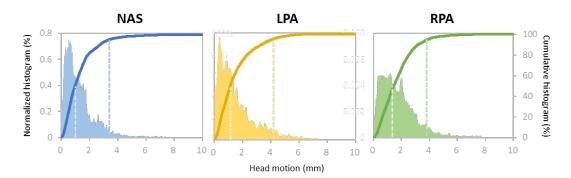
All preprocessed data were deposited in the "preproc meg-mne mri-fmriprep" 268 subdirectory under the "derivatives" (Fig. 3c). The preprocessed data of each 269 270 participant were separately saved in the "sub-<participant id>/ses-movie" directory, which contains two subfolders, namely "anat" and "meg". The "anat" folder 271 272 comprised the preprocessed MRI volume, reconstructed surface, and other associations, including transformation files. The "meg" folder included preprocessed 273 MEG recordings, including "* meg.fif.gz", "* ica.fif.gz" and "* decomposition.tsv", 274 and "* trans.fif" for the preprocessed data, ICA decomposition, and MEG-MRI 275 coordinate transformation, respectively. In addition, the FreeSurfer surface data, the 276 high-resolution head surface ("freesurfer/sub-<participant id>/bem/*"), and the MRI-277 fiducials ("freesurfer/sub-<participant id>/bem/*fiducials.fif") were provided in 278 "freesurfer/sourcedata" directory for MEG-MRI coregistration. 279

280 Technical Validation

We assessed the data quality of both the raw and preprocessed data using four measures as follows: head motion magnitude, stimuli-induced time-frequency characteristics, homotopic functional connectivity (FC), and inter-subject correlation (ISC).

285 Motion magnitude distribution

Head movements during MEG scans are one of the significant factors that 286 degrade both sensor- and source-level analyses. Herein, we calculated the motion 287 magnitude for each sample as the Euclidian distance between the current and the 288 initial head position while the movie segment began playing. The head motion across 289 all runs and all participants were summarized for each of the three fiducials (NAS, 290 LPA, and RPA) to provide an overview of the head movement of the dataset. As show 291 in Fig. 4, motion magnitude of 95% of the samples had head motions lower than 3.43 292 mm, 4.11 mm, and 3.87 mm for NAS, LPA, and RPA, respectively. Furthermore, 50% 293 of the samples had head motions smaller than 0.99 mm, 1.10 mm, and 1.46 mm for 294 NAS, LPA, and RPA, respectively. These findings indicated low head motion 295 magnitude on average. The head motion magnitude of each participant could be found 296 297 in Supplementary Fig. 1. 298



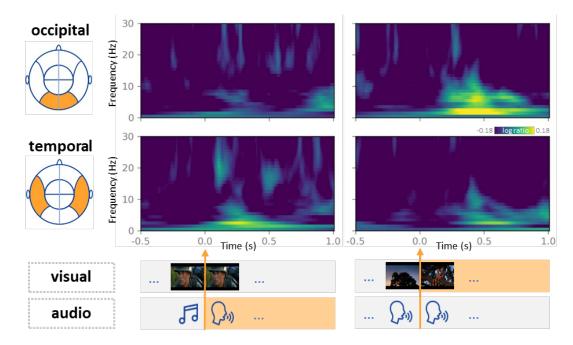
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Fig. 4. The ensemble distribution of head motion magnitude across all runs and
all participants. The density and accumulative histogram of motion magnitude of all
samples from all acquisitions for three fiducials (NAS, LPA, and RPA) have been
plotted. The dashed lines indicate the 50% and 95% of the cumulative density. Left Yaxis: normalized histogram; Right Y-axis: cumulative histogram.

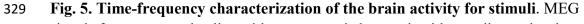
306 Time-frequency characterization of brain activity

Herein, we validated whether MEG recordings could successfully detect the change in stimuli-induced brain activity. Because the movie stimuli do not have explicit condition structures as in conventional design, we selected two exemplar movie clips, within which the audio or visual features showed pronounced changes to examine if the expected change in MEG signals could be detected at the related sensors. In one clip (Seg 3: frame 15864 ± 125), the audio features changed

significantly (a vocal voice developed from background music) whereas the visual 313 features were stable. In contrast, the other clip (Seg 1: frame 21768 ± 125) comprised 314 stable audio features, whereas the visual features changed from landscape to human 315 figures. Validation was performed according to the following procedure^{25–27}: First, 316 time-frequency analysis with Morlet wavelets was conducted for each sensor in the 317 occipital and temporal lobes. The baseline was set to 1000 ms before the change 318 points of the audio or visual features, and the baseline mean was subtracted for each 319 channel. Second, the time-frequency representations were averaged across the 320 participants. Finally, the time-frequency representations were averaged across the 321 sensors from the occipital and temporal lobes, respectively. As shown in Fig. 5, the 322 time-frequency representations from the occipital sensors, and not the temporal 323 sensors, were locked with changes in visual features. The opposite pattern was 324 observed for the audio feature changes in the stimuli. The results demonstrated that 325 current MEG data could accurately detect stimulus-induced brain activity. 326 327



328



signals from two movie clips with pronounced changes in either audio or visual 330

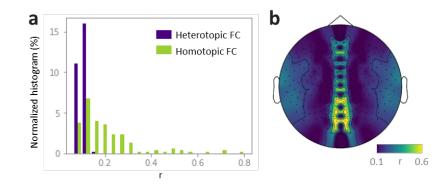
features of the stimuli have been examined. The occipital sensors (top) display 331

332 significant signal changes with a change in the visual features of the stimuli. The

- temporal sensors (bottom) display significant changes with a change in the audio 333 features.
- 334

336 Homotopic functional connectivity

A basic principle of the brain's functional architecture is that FC between 337 inter-hemispheric homologs (i.e., homotopic regions) is particularly stronger than 338 other interhemispheric (i.e., heterotopic) FC^{28,29}. Herein, we tested if MEG data for 339 dynamic movies at the sensor level could reveal strong homotopic FC. First, we 340 calculated the absolute envelope amplitude of the MEG signal from each sensor via 341 the Hilbert transform and down-sampled to 1 Hz. Second, the sensor-level homotopic 342 FC was calculated using Pearson's correlation between the envelope amplitude of 343 each homotopic sensor pair. For comparison, the heterotopic FC was also calculated 344 for each sensor as the average correlation between all heterotopic sensor pairs. Finally, 345 the homotopic and heterotopic FC values were averaged across all runs and all 346 participants. The homotopic sensors expectedly revealed stronger FC than the 347 348 heterotopic sensor pairs (Fig. 6a). Moreover, the high homotopic FC primarily appeared at the sensors located in the occipital and temporal cortices, thereby 349 350 indicating strong couplings driven by the movie stimuli (Fig. 6b). 351



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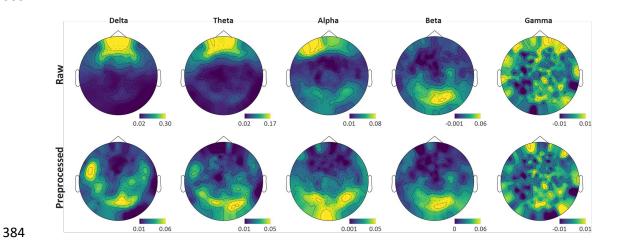
Fig. 6. The sensor-level homotopic functional connectivity (FC) is stronger than
the heterotopic FC. (a) The histogram of the sensor-level homotopic FC and
heterotopic FC pooled across all runs and participants. (b) The topographic map of the
sensor-level homotopic FCs averaged across all acquisitions. Identical homotopic FC
values are displayed for the corresponding homotopic sensors from the two
hemispheres. Sensors in the central axis with no corresponding homotopic sensors
were not included in the analysis.

361 Inter-subject correlation

362 ISC analysis uses the brain responses of a subject to naturalistic stimuli as a 363 model to predict the brain responses of other subjects³⁰. Numerous studies have

demonstrated that visual and auditory cortices display significant ISC while watching 364 audio-visual movies. We validated if a high ISC could be detected in our MEG data. 365 366 For simplicity, the ISC analysis was conducted at the sensor-level. The MEG recordings captured neural oscillations at different frequency bands³¹. Therefore, the 367 368 ISC was calculated in five bands (delta: 1-4 Hz, theta: 4-8 Hz, alpha: 8-13 Hz, beta: 13-30 Hz, and gamma: 30-100 Hz). First, the MEG signal was filtered for each band. 369 Second, the absolute envelope amplitude of each band was calculated via the Hilbert 370 transform and down-sampled to 1 Hz. Third, for each frequency band, a leave-one-371 participant-out ISC was calculated for the left participant as the temporal correlation 372 between the envelope amplitude from the participant and the average of other 373 participants. Finally, the mean ISC was calculated by averaging the ISC across all 374 participants. As shown in Fig. 7, sensors with higher ISC were located near the visual 375 and audio cortices, which reportedly displayed high ISC during movie watching in 376 previous studies^{14,32–34}. In particular, the high ISC predominantly occurred in the delta, 377 theta, and alpha bands, consistent with previous studies^{14,33,34}. Together, the dataset 378 demonstrated good validity in detecting ISC. In addition, a high ISC was observed in 379 the orbital frontal area in the raw data, likely caused by eye blink or movement 380 considering that high ISC was not observed in the preprocessed data, in which the 381 artifacts have been removed. 382

383



385

Fig. 7. Topographic maps of ISC in different frequency bands derived from both
the raw and preprocessed MEG data. A high ISC occurs near the visual and audio
cortices in the delta, theta and alpha bands for both the raw (top) and preprocessed
(bottom) MEG data. A high orbital frontal ISC is only observed in the raw data, likely
caused by artifacts.

392 Usage Notes

We presented the first public MEG dataset for a full-length movie. The MEG 393 signals were recorded while the participants watched the 2 h long Chinese-dubbed 394 audio-visual movie "Forrest Gump". The dataset provided a versatile resource for 395 studying information processing in real-life contexts. First, MEG data could be 396 independently used to study the neural dynamics of sensory processing and higher-397 level cognitive functions under real-life conditions. Second, as a studyforrest 398 399 extension, the dataset could be integrated with publicly available fMRI data from the 400 studyforrest project. The fusion of fMRI and MEG may shed new light on the 401 relationship between spatially localized networks observed in fMRI and the MEG-402 derived temporal dynamics. Moreover, our massive MEG recordings enable the direct training of DNNs with neural activity patterns. In contrast to the DNNs that were 403 404 usually trained with stimuli without referring to any neural representation, this kind of brain-constrained DNNs would act more like the human brain and generalize well 405 across many tasks^{35,36}. 406

Despite the importance of the aforementioned dataset as an extension of the 407 studyforrest dataset in studying the spatiotemporal dynamics underlying cognitive 408 processing in real-life contexts, the limitations should be acknowledged. First, the 409 participants in our MEG data did not overlap with that in the studyforrest project. 410 Therefore, the fMRI-MEG fusion can be only performed at the group level (i.e., 411 across participants) instead of the individual level (i.e., within participants). This may 412 make it unable to study the individual differences in the coupling between spatially 413 localized networks and temporal dynamics. Second, the dubbed languages used in our 414 dataset and the studyforrest project were radically different, thus limiting the 415 application of the data in examining spatiotemporal dynamics of brain activity 416 underlying auditory and language. In addition, caution should be taken with timing 417 differences between the stimuli in the MEG and fMRI data. Considering the lower 418 419 sensitivity of fMRI signals to the exact timing than MEG signals, we recommend the use of MEG stimuli in fusing fMRI and MEG data. 420

421

422 Code Availability

423 All custom codes for data preprocessing and technical validation are available 424 at <u>https://github.com/BNUCNL/MEG_Gump</u>. Preprocessing was performed using

- 425 MNE-BIDS (https://mne.tools/stable/index.html), MNE
- 426 (https://mne.tools/stable/install/mne_python.html), fMRIPrep
- 427 (<u>https://fmriprep.org/en/stable/</u>), pydeface (https://github.com/poldracklab/pydeface),
- 428 and dcm2niix (https://github.com/rordenlab/dcm2niix).
- 429

430 Author contributions

- X.L. conceived, performed the study, and wrote the manuscript. Y.D. performed
 the study. H.X. contributed to the data collection. Z.Z. conceived, supervised the study
 and wrote the manuscript.
- 434

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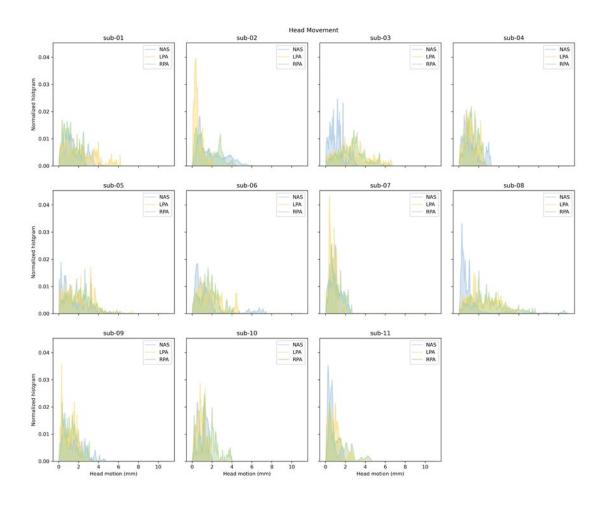
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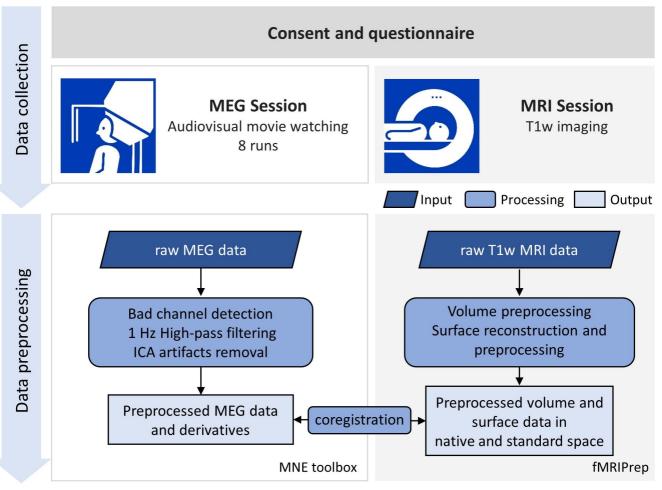
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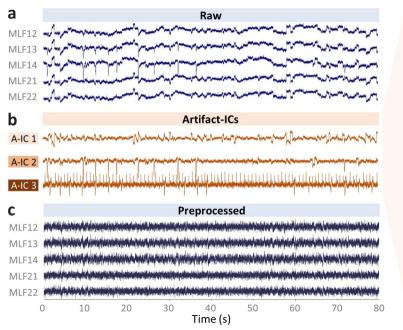


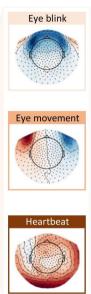


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Supplementary Figure 1. Head motion magnitude from each individual participant. The
density histogram of motion magnitude calculated for three fiducials (NAS, LPA, RPA)
were plotted for all samples, across all runs for each participant.







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