Anti-clotting functions of lymphatics form the natural on-off switch for immune recognition by controlling the antigens and immune cells access to the lymph nodes

Witold W Kilarski[1,2,✉,Ω], Małgorzata Wachowska[3], Angelika Muchowicz[3], Renata Mezyk-Kopec[4], Jakub Gołąb[3] & Melody A Swartz[1,2,5,✉,Ω]

The ability of lymph to clot indicates that similar to blood vessels lymphatics must have means to counteract this process. We analyzed their hemostatic properties, tailoring them for the potential therapeutic applications. Inflammatory stimuli induced tissue factor-dependent focal lymph clotting while blocking thrombomodulin lead to widespread but also transient occlusion of collecting vessels. Decellularization of lymphatics resulted in tissue factor-independent lymphatic occlusion by widespread and persistent lymph clots. These decellularized basement membrane remnants of collectors were capable of macromolecules drainage and leukocytes transit only when lymph clotting was inhibited with heparin. In occluded 'ghost' vessels, fibrin was replaced with transient basement membrane-rich inclusions to be eventually reperfused. During regeneration, ghost vessels were filled with granuloma-like clusters of antigen-presenting and T cells. Despite that, immune response against allografts placed under non-drained skin was not developed as long lymphatics remained occluded, and graft survival was prolonged together with the delay of lymphatic regeneration with anti-lymphangiogenic therapy. Other potential applications of lymphatic hemostatic control functions include blocking pathogen or metastasis spread but also should be considered in the treatment of lymphedema.

Intima lining of blood vasculature forms the only known surface that is able to control blood liquidity[1] dynamically, and despite ontogenetic and functional similarities, that function has not been yet ascribed to its relative circulation of lymphatic vessels. However, since the first description of the lymphatic system by Olaf Rudbeck over 350 years ago, lymph is known for its ability to coagulate when stored outside of the lymphatic vessels (discussed in[2,3,4]). Interestingly, the above references illustrate that most of the research on lymph clotting was conducted over 50 years ago with little impact on the understanding of lymphatic related pathologies or therapeutic application [5]. Indeed, even though lymph clotting time is delayed as compared to blood, it has intrinsic clotting properties[6, 78]. Its clotting time varies in a broad, up to 20-times range as a concentration of lymph clotting factors that fluctuate between species, individuals or even sampling location, and is 10 to 70% lower as compared to the blood[9-11]. Together with the absence of platelet-derived anionic phospholipids required for activation of Xase and prothrombinase and a higher concentration of fibrinolytic factors assure lymph hypercoagulability under physiological conditions[8, 12]. Also, due to the lack of thrombocytes, lymph, in contrast to blood clots, do not retract[8]. On the other hand, relatively slow lymph flow and possibility to substitute platelet phospholipids with membrane components of endothelial cells[13] may favor lymph clotting for example, during inflammation, when augmented blood vessel permeability to plasma proteins leads to 3-fold enrichment of plasma proteins in interstitial fluid and lymph [14]. While data are missing for the inflammation or injury-driven concentration change of individual clotting factors in the lymph, it is rather safe to assume that concentration of coagulation components would rise when the rate of protein extravasation from blood vessels increases up to 100 times normalvcv[2, 15, 16].

These observations confirm that lymph is a hemostatic fluid, but more importantly, it infers that similar to blood vessels, lymphatics must have specific anti-coagulatory properties that enable them to control lymph fluidity. By doing so, the lymphatic system could regulate other passive functions of lymphatics, i.e., fluid drainage and cell trafficking, and similar to blood vessels use pro-hemostatic mechanisms to limit the spread of infections[17]. However, only a handful of studies address thrombo-regulatory properties of lymphatic endothelium (for review see[12]). For example, it was shown that similar to blood endothelial cells; lymphatic collectors express thrombomodulin, a membrane receptor capable of switching the substrate specificity of thrombin to protein C, thus making thrombin a potent anticlotting factor [18]. On the other hand, lymphatic endothelium does not produce von Willebrand factor, a multimeric protein that participates in platelet activation on the exposed subendothelial collagen. This phenotype, however, is in line with the lack of platelets in lymph[19].

In response to pro-inflammatory molecules such as cytokines TNFα, IL-1β or TLR agonist LPS, blood endothelium can turn into a pro-thrombotic surface, e.g., by initiating the expression of tissue factor (TF), membrane receptor initiating extrinsic coagulation pathway[20]. Few in vitro studies have demonstrated that lymphatic endothelial cells are also capable of responding to inflammatory stimuli, for example with increased synthesis of plasminogen activators and inhibitors[12, 21].

[1]Pritzker School of Molecular Engineering, University of Chicago, IL, USA, [2]Institute of Bioengineering and Swiss Institute for Experimental Cancer Research (ISREC), École Polytechnique Fédérale de Lausanne (EPFL), Switzerland, [3]Department of Immunology, Center of Biostructure Research, Medical University of Warsaw, Poland, [4]Ben May Department for Cancer Research, University of Chicago, Chicago, IL, USA. [Ω]These authors jointly supervised this work.✉To whom correspondence should be addressed: witek.kilarski@lymphatic-research.org or melodyswartz@uchicago.edu.

B

0	30 min	6 hours	6 hours 30 min	20 hours
i.d. TF-I	i.v. FITC-fibrinogen	i.d. TF-I	i.v. FITC-fibrinogen	Image, Perfuse & Fix

C TNFα   TNFα and IL1β   thrombin^in/ac

D Day 0   Day 1   Day 1

dextran   fibrin

thrombin^in/ac

Control

E th^ac/in TNFα IL1β   th^ac/in TNFα IL1β   **F** αTF + th^ac/in TNFα IL1β

dextran fibrin

live   exposed   exposed

Figure 1. Inflammatory mediators lead to lymph coagulation and block the fluid drainage in discrete segments of lymphatic collectors. A. Left: The pattern of thrombomodulin expression overlapped with the expression of endothelial marker CD31 but was also present on some *perivascular* and interstitial cells but also within nerve fibers (n). Arrows point to collecting lymphatics that have unique morphological features, i.e., the presence of valves with uneven vessel diameters. **Middle:** In non-inflamed ear skin, endothelial cells of lymphatic collectors (LECs) similar to blood endothelium (BECs) express thrombomodulin but not tissue factor (TF), whose expression is restricted to perivascular cells and adipocytes (a). **Right:** In contrast to BECs, LECs did not accumulate the von Willebrand factor. **B.** Schematic of experimental design. Intradermal injection of tissue factor inducers (TF-I: TNFα, TNFα, and IL1β or thrombin^in/ac - partially inactivated thrombin, see methods) on day 0 was followed by intravenous injection of fluorescently labeled fibrinogen. Six hours after the first injection, the procedure is repeated. The mouse is perfused and fixed 13 hours later. **C.** Two subsequent remote intradermal injections of TF-I TNFα, TNFα, and IL1β or partially inactivated thrombin (thrombin^in/ac, a mix of proteolytically inactive and active thrombin; 6:1 ratio) resulted in the formation of intralymphatic clots within specific locations of lymphatic collectors as shown by the presence of fluorescent fibrin. Basement membrane was stained by collagen IV. **D. Top:** Demonstration of lymphatic drainage by intradermal injection of fluorescent dextran. Two consecutive injections (6 hours apart on day 1) of thrombin^in/ac blocked lymphatic drainage in some branches of the collecting lymphatic network 12 hours after the second injection. Intralymphatic clots (fibrin) are present in with the location of lymphatic collector junction functional lymphatic was blocked (arrows). **Bottom:** Intradermal injections of PBS had no adverse effect on lymphatic perfusion. Arrows point to collectors that were blocked by intralymphatic fibrin (green). Arrowheads mark the same functional vessels visualized on the day of the experiment (Day 0) and the following day. **E. Left:** Superficial view of the live dorsal skin of the ear after lymphangiography. Combination of all three pro-clotting factors in single treatment had no cumulative effect and, similar to the individual-factor treatment, induced lymph clotting that blocked vessel drainage only in certain collectors. th^at/in – partially inactivated thrombin. **Middle:** Internal view of the same ear skin after the mouse was fix-perfused and dorsal skin exposed by detaching ventral skin flap with cartilage. Arrowhead and arrow point to the same vessel locations. **Right:** Internal view of the exposed dorsal dermis where lymph clotting was prevented with co-injection of tissue factor-blocking antibody (αTF). The intensity of the von Willebrand factor was normalized to its signal level in capillaries. The intensity of lymphatic fibrin deposits was normalized to the signal level of clots at the sites of injection (*). Scale bar: **A, C** – 50μm, **D, E** – 250μm.collectors, and TF expression was reduced or absent on lymphatic endothelial cells. Arrows point to fibrin clots, arrowheads, MHCII-positive antigen presenting cells. **L** marks lymphatic collectors. TF intensity was normalized to the TF expression level of interstitial cells. Note that lymph clots are autofluorescent in the red channel due to cross-reactivity of anti-rat antibody with clot-entrapped mouse IgGs, hence the TF signal can be appreciated only at the edges or outside the clot. Scale bar: 50μm.

In contrast to blood circulation, where vessel occlusion by thrombus leads to tissue ischemia and immediate localized symptomatic pain, development of edema that follows lymphatic blockage can take a long time and still remain undetected[22]. Yet, there is clinical evidence of pathological lymph clotting that accompanies certain inflammatory pathologies. For example, intralymphatic lymph clots encapsulating the granuloma were found in the chronic inflammation[23], surrounding dead worms in lymphatic filariasis[24, 25] or occluding vessels in patients with idiopathic primary lymphedema[26] or secondary lymphedema [27]. These clots often undergo fibrosis, forming long-lasting intravascular intrusions in chronic diseases [23, 25, 27]. The tumor microenvironment is another typical inflammatory pathology, where leaky blood vessels and chronic inflammation should constitute ideal conditions for intravascular lymph clotting. Indeed, biomarkers of tumor stroma, i.e., TF overexpression, interstitial fluid hypercoagulability and stromal fibrin deposition[28, 29] correlate with dysfunctionality or complete occlusion of intratumoral lymphatics in most human cancers[30]. However, fibrin as a provisional matrix undergoes rapid digestion or fibrotic remodeling[31] while pre-symptomatic tumor development is a chronic disease that can take years to develop. Therefore, it is not surprising that there are only scant reports describe fibrotic occlusion of lymphatics associated with human tumors[32] or identified by us lymphatic fibrosis in an experimental mouse model of B16-F10 melanoma (**Supplementary Fig. 1**).

The transport of clottable lymph requires anchoring of anti-clotting mechanism in the walls of lymphatic collectors but also creates an opportunity for lymphatic endothelium to change lymphatic patency depending on tissue condition dynamically. Hence, we suspected that lymphatic endothelium is critical to sustaining patent lymphatic collectors but also that it could induce lymph clotting by, e.g. TF expression alone or in collaboration with leukocytes accumulating within lymphatics during inflammation. In that case, it should be possible to reverse potential anti-hemostatic properties of lymphatics with pharmacological inhibition of thrombomodulin, turning lymphatic endothelium into a pro-thrombotic surface with the expression of pro-thrombotic tissue factor (TF) or decellularization of lymphatic collectors, which not only removes the endothelial source of anti-thrombotic factors (thrombomodulin, plasminogen activators) but also expose negatively charged basement membranes, which laminin and collagen I[33]can activate intrinsic coagulation pathway[34]. We verified that challenge-induced formation of intravascular lymph clots primarily relied on the physiological state of the endothelium rather than the presence of infiltrating leukocytes. Finally, we showed that intact lymphatic endothelium is indispensable for the sustenance of lymphatic patency but not lymph and immune cell transport through collecting vessels. As a proof that anti-clotting function of lymphatic endothelium can be applied therapeutically, we showed that complete block of lymph transport to the draining lymph node delayed immune response against subcutaneous allograft until the recovery of decellularized lymphatics. Blinding the lymph node to antigens lead to their ignorance by the immune system, a local treatment that can be used to prolong the survival of allografted cells or tissues without systemic and toxic immunosuppression.

Results

Induced TF expression on lymphatics leads to lymph clotting and obstruction of drainage

Here we analyzed the anti-clotting properties of lymphatics and the means to control them. In a normal physiological state the endothelium of lymphatic collector, similar to blood endothelial cells, express anti-thrombotic thrombomodulin receptor but do not express tissue factor (**Fig. 1A**). However, contrary to blood endothelium, lymphatic collector endothelium is not expected to encounter platelets, and consequently, they lack the intracellular stores of von Willebrand factor, the critical factor for platelet adhesion to the subendothelial collagen at the location of vascular wounds. Stimulation of de novo expression of tissue factor on lymphatic endothelial cells appeared as the most intuitive and feasible approach. We assayed the activation of intralymphatic coagulation in mouse skin by posttreatment intravenous injection of fluorescently labeled fibrinogen (**Fig. 1B**). If fibrinogen that leaked to the tissue was polymerized into insoluble fibrin, its fluorescent deposits could be detected with intravital microscopy of thin mouse ear or, after fixation, in the whole mount preparation with confocal optical sectioning.

TNFα and IL1β are cytokines known as potent inducers of tissue factor (TF) expression in vitro[20, 35] but only on subsets of blood endothelial cells in vivo[36]. Inflammatory stimulation of TF on the intima layer of blood vessels results in activation of the extrinsic pathway within vessel lumen and temporary, local vessel occlusion by thrombus. Similar in lymphatics, even in the absence of platelets, repeated intradermal injections of TNFα induced clot formation within draining collectors but only at discrete locations (**Fig.1C**). No cumulative effect was observed when TNFα was co-injected with IL-1β, and this treatment produced a similar sparse distribution of clots within collectors. Activation of G-protein coupled receptor PAR-1 with thrombin acts synergistically with TNFα on TF expression on blood endothelium[37] and that treatment has the potential to augment the effect of the cytokine. Surprisingly, injection of 2.5 IU thrombin alone had no effect on intralymphatic coagulation away from the site of injection but as expected led to massive coagulation within blood vessels (**Supplementary Figure 2A**). However, we found that treatment of thrombin with small-molecule covalent inhibitor phenylmethanesulfonyl fluoride (PMSF) inactivated 80% of the enzyme (six-times times longer clotting time). Similar to cytokines treatment, recurrent intradermal injections of the mix of partially inactivated thrombin (thrombin^in/ac) induced the formation of intralymphatic clots within specific locations of lymphatic collectors without the bystander coagulation within blood vessels circulation (**Fig 1C and Supplementary Fig 2B**). Injections of thrombin diluted to 0.5 IU concentration resulted again in coagulation within blood vessel over the lower surface of the skin but had no effect on intralymphatic clotting (not shown) suggesting that inactive thrombin had an effect on lymph clotting. Even though fibrin was deposited only in few collector branches (but always in at least one collector segment in all 9 tested ears), their formation was sufficient to occlude lymphatic drainage from all lymphatics efferent to that collector (**Fig. 1D**). Against our expectations, there was no cumulative effect of combined treatment with cytokines and thrombin on lymph clotting and similar to injection of individual factors only discrete locations in collectors were functionally occluded with fibrin clots. Occlusion induced by the mix of partially inactivated thrombin (**thromb^in/ac, Fig. 2A**) or a mix of TNFα and Il-1β cytokines and thromb^in/ac (**Fig. 1E, Fig. 2B**) could be prevented with TF blocking antibodies. Confocal images of fibrin-occluded lymphatics stained for TF revealed that lymph clotting co-localized with high expression of TF on lymphatic endothelium. These results indicated that thrombin does not induce lymph clotting directly but instead it activates certain cell clusters in divergent endothelium of collectors. Heterogeneity of TF expression resembles the similar discontinuous pattern of CCL21 expression previously reported by our group[38] but is also characteristic for blood endothelial cells where TF density on the cell surface varied strongly among TNF-alpha-stimulated endothelial cells in vitro[20] and in vivo[36, 39]. Combined treatment with cytokines and thrombin^in/ac had a cumulative effect on dendritic cells (DCs) immigration to lymphatics. In contrast, either due to faster transmigration, stimulated cell death or inhibition of migration of DCs to lymphatics, DCs were absent from intralymphatic cloths in triple-factor stimulated lymphatics but filled the lymphatic along the high TF expression zone in thrombin^in/ac treated skin (**Fig. 2B**). This lack of co-localization of intralymphatic DCs and lymph clots but also a weaker expression of TF (**Fig. 2A inset**) as compared to activated lymphatics indicated that lymphatic endothelium-derived TF was

sufficient to induce clot formation. Inhibition of anti-clotting pathway by thrombomodulin blocking leads to instant dissipated intralymphatic lymph clotting.

There is a low basal level of tissue factor-dependent activation or 'idling' of the clotting system in normal individuals resulting in a constant, low level of formation of thrombin. In the absence of an anti-clotting mechanism, the activation threshold of clotting cascade is crossed, and clotting cascade is initiated[40, 41]. The necessity of co-injection of mixed active and inactive thrombin to initiate lymph clotting suggested that inactivated thrombin served a role in activation of lymph clotting. Thrombin has two types of receptors on endothelial cells, thrombomodulin and protease-activated G-coupled receptors (PAR-1 on endothelium)[39]. PAR-1, however, has to be activated by thrombin proteolytic cleavage, hence inactivated thrombin cannot initiate its signaling. On the contrary, thrombin binding by thrombomodulin is independent on its enzymatic state when inhibited by small molecular inhibitors at thrombin active site[42]. Thrombomodulin-bound thrombin shifts its enzymatic specificity from fibrinogen to protein C, which activation, in turn, leads to the destruction of co-factors V and VIII and inhibition of clotting process[18]. Hence, blocking thrombin binding sites on thrombomodulin can inhibit the whole anti-clotting pathway. Treatment of thrombin with the potent, small-molecule covalent inhibitor p-(amidonophenyl) methane sulfonyl fluoride (APMSF) inactivates 99.75%

Figure 3. Completely inactivated thrombin blocks lymphatic drainage. A. Schematics of experimental design. Intradermal injection of saline, active thrombin (thrombin^ac) or completely inactivated thrombin (thrombin^in) was followed by intravenous injection of fluorescently labeled fibrinogen. The mouse is fixed by perfusion 13 hours later. **B. Top:** Lymphangiography and intra-lymphatic fibrin in collectors of live tissue 5 hours after intradermal injection. **Bottom.** Imaging of fluorescent insoluble fibrin clot in fixed-perfused dorsal skin flap after cartilage and ventral skin were removed. Two adjacent injections of 2.5 µl PBS had no effect on the collector-drainage later (**PBS, top**). Fibrin formed only in the interstitium at the injection sites (**PBS, bottom**). Active thrombin (2.5 IU; thrombin^ac) increased hyperpermeability of collectors but did not block their drainage (**Top, thrombin^ac**). Fibrin formed within blood vessels around the site of injection (**Bottom, thrombin^ac**). In contrast to thrombin^ac, intradermal injection of inactive thrombin (thrombin^in) occluded remote lymphatic collector vessels (**Top, thrombin^in**). Drainage discontinuities visible on lymphatic

lymphangiography are bridged by green fibrin deposits, indicating an incomplete occlusion. In contrast to continuous fibrin clots induced in blood vessels by thrombin^ac, thrombin^in induced the formation of discontinuous clots in a large number of remote lymphatic collectors but had no effect on plasma coagulation in blood vessels (**Bottom thrombin^in**). **C.** Higher magnification confocal images 5 hours after the second injection of compounds indicated in B. Collagen IV stained lymphatic collectors (L) and blood vessels (Bl) identified by their characteristic morphology (valves, uneven diameter along the vessel length). In PBS injected mice, fibrin clots were not formed away from the injection site. CD31 showed normal cell-cell junctions between lymphatics (**PBS**). Active thrombin blocked blood circulation, trapping autofluorescent erythrocytes (yellow) within blood vessels (**Bl**) around the injection site. Rare intralymphatic clots (**L**) could be found only around the thrombin^ac injection site (**Thrombin^ac**). In the **Thrombin^in** injected skin, discontinued fibrin clots in remote lymphatic collectors were observed. **D. Top.** 16 hours after injection of **PBS**, tissue plasminogen activator (TPA) is randomly distributed within the skin but is also stain morphologically distinct macrophages (M)., erythrocytes trapped within blood vessels, TPA-positive macrophages but also large vessels were seen around the site of **Thrombin^ac** injection. In the skin injected with **Thrombin^in**, TPA strongly labeled collecting lymphatic vessels filled with residual, centrally-located fibrin clots. **Bottom.** Imaging of the same field stained with collagen IV depicted tissue stationary structures, i.e., blood vessels, lymphatics, and adipocytes. A-adipocytes, L-lymphatic collectors, Bl-blood vessels, M-macrophages, Hf-hair follicle. The intensity of TPA was normalized to its signal level in interstitial cells. The intensity of lymphatic fibrin deposits was normalized to signal level of clots at the sites of injection (*). Scale bar: B–500 µm, C-50µm.

of the enzyme[43] and in our hands, it prolonged 400-times times the clotting time. A single injection of saline had no effect on lymph clotting or dextran drainage (**Fig 3A-B**) and draining lymphatics preserved normal cell-cell junctions. Fully active thrombin-induced coagulation within blood vessels at the site of injection but had no effect on lymph clotting in remote lymphatics. APMSF-inactivated thrombin-induced lymph clotting in most segments of draining lymphatic collectors. However, due to incomplete lumen occlusion and rapid dissolution of these clots, intralymphatic clots only partially inhibited the lymphatic drainage, the blockage could be overcome with pressurized syringe injection. Inactive thrombin injected skin, intralymphatic fibrin clots could be found only

around the site of the injection together with blood vessel clots entrapping autofluorescent erythrocytes within blood vessels (**Fig. 3C**). Fast dissolution of intralymphatic clots (after injection of inactive thrombin, thrombin[in]) could be explained by increased expression of tissue plasminogen activator by lymphatic endothelial cells. Indeed, 16 hours after injection of thrombin[in], lymphatic collecting vessels emerged from other tissue structures by an elevated level of TPA expression (**Fig. 3D**). Active thrombin (thrombin[ac]) at the site of injection-induced larger tissue damage and robust activation of TPA in various tissue cells, i.e., adipocytes, macrophages and also blood vessels, making these structures to stand out from surrounding tissue. In regular non stimulated tissue TPA was mostly expressed by macrophages, but with the exception of hair follicles, no stationary structures could be identified by distinctive TPA expression. A similar mechanism might be responsible for fast clearance of lymph clots in inflammatory factor-treated lymphatics where we also observed a high level of TPA expression within stimulated lymphatics (not shown). Intradermal clot deposited in the skin outside blood vasculature remains within the skin in roughly unchanged shape for at least 24 hours (**Fig. 4A**). In contrast, thrombin[ac]-induced blood vessel clots were almost entirely cleared from clot formation by thrombomodulin blocking lost its dependency on TF after tissue pre-injection with TF-blocking antibodies. This possibility was excluded as we showed that mock pre-injection or injection with TF-blocking antibodies and subsequent injection of skin with TF-blocking antibodies and thrombin[in] did not inhibit the circulation. Re-injection of saline and thrombin[ac] re-created clots in dermis and blood vasculature, respectively.

Figure 4. Completely inactivated thrombin instantly but transiently occlude lymphatic collectors by a tissue factor-independent mechanism. Intravital imaging of fluorescent fibrin clot formation within the ear skin vasculature. Fluorescent fibrinogen was administered i.v. immediately after 2.5 µl intradermal injection of indicated compounds in two adjacent injection sites on a single ear dorsal dermis. In all images, lymphatics drain from the right (distal) to the left (proximal). The functional blood vessels appear dark in all images as tissue was fixed by perfusion to clear the vessels from non-coagulated fibrinogen. **A.** Top: Injections of PBS result in injury of blood vessels, plasma leakage, and clot formation within the dermis, which was restricted to immediate surroundings of injection spots. Middle: Injections of active thrombin (thrombin[ac], 2.5 IU) resulted in coagulation in blood vessels, blood vessel leakiness, and fibrin clotting within the area of the ear when injection edema formed. Intravascular and interstitial clots were largely cleared within 24 hours after the injection, however, they could be re-created with another intradermal injection of active thrombin[ac]. **Bottom**: Similar to PBS injections, a single dose of partially inactivated thrombin (thrombin[in/ac]) caused leakage of plasma and intradermal fibrin clotting around the site of injection but had no effect on blood or lymphatic vasculature. However, reinjection of thrombin[in/ac] 24 hours later induced the formation of intralymphatic clots at discrete lymphatic locations, downstream to the sites of injection. Arrows point to single intralymphatic clots defined by their sharp edges, in contrast to the whole lymphatic that is visible due to non-coagulated fibrinogen labeled lymph. **B.** Ears after injection with thrombin[in] inactivated with APMSF (400-fold decrease in activity, thrombin[in]). **Top**: Single dose of thrombin[in] (co-injected with irrelevant rat antibodies) resulted in rapid formation of fibrin clots within most draining lymphatic collectors, which were mostly cleared 22 hours later. Reinjection of thrombin[in] re-created clotting pattern within lymphatics. Arrowheads point the same intralymphatic clots visible at 2 and 24 hours after first injection and 5 hours after the second injection. **Bottom**: Co-injection of tissue factor-blocking (αTF) antibodies and thrombin[in] did not inhibit instant intralymphatic clot formation, however reinjection of αTF and thrombin[in] 24 hours later did not induce the formation of intralymphatic clots. **C.** Neither pre-injections with PBS (injection injury) nor αTF antibody (day 1) inhibited intralymphatic clot formation induced with thrombin[in] or with thrombin[in] and αTF co-injection on day 2 at 24 hours after the first injection. Images were taken from ears fixed 5 hours after the second injection. The intensity of CD31 was normalized to its signal level in the lymphatics draining control region. The intensity of lymphatic fibrin deposits was normalized to the signal level of clots at the sites of injection (*). Scale bar: 250µm.

In contrast, the effect after the first injection of thrombin[in/ac], partially inactivated with PMSF resembled injection of saline. Only the second injection Also, a large number of rounded inflammatory cells infiltrated t of thrombin[in/ac] 24 lymph clotting (**Fig. 4C**). Instead, it seems likely that initial activation of clotting pathway leads to sensitization to the extravascular TF by shifting the intralymphatic hemostatic balance to fibrinolytic, where activated endothelial cells upregulate production of TPA (**Fig. 3D**). In that scenario, idle extravascular TF activity or contact activation pathway initially suffice for the accumulative lymph clotting and become insufficient in the presence of high levels of plasmin.

Noxious agents kill endothelium that leads to lymph clotting completely occluding lymphatic collectors

Necrosis of endothelial cells within lymphatic collectors

leads to localized sterile inflammation that should have multifactorial pro-hemostatic effects on the transported lymph[44]. First, the elimination of thrombomodulin anti-clotting mechanism inherently linked to lymphatic endothelial cells promotes amplification of contact-dependent pathway on exposed RNA and polyphosphates from dying cells[45]. Also, decellularization of the lymphatic surface should prolong the occlusion of lymphatics as it eliminates the source of endothelium-derived tissue plasminogen activator[46] that is a cause of the fast clearance of intralymphatic clots from TF-expressing or thrombomodulin blocked lymphatics (**Fig. 3E**). Finally, sterile inflammation leads to infiltration of TF-expressing hydroxyl and hydroperoxyl radicals from mitochondria-derived hydrogen peroxide and it is used in TF-independent blood vessel thrombus formation models[48]. Intradermally hours after the first injection induced lymph clotting in discrete and remote to injection sites lymphatic segments. Thrombin[in] completely inactivated with APMSF induced dissipated fibrin clotting in most collectors already 2 hours after the injection. Similar to in the case of blood vessels, most intralymphatic clots were cleared 22 hours later (**Fig. 4B**). First co-injection of thrombin[in] with TF-blocking antibody did not inhibit intralymphatic clot formation. Unexpectedly, re-injection of TF-blocking antibodies 22 hours later completely blocked thrombin[in]-dependent intralymphatic clot formation, suggesting that activated monocytes that could directly induce lymph clotting by extrinsic pathway[47]. To induce sterile inflammation of collecting vessel endothelium we choose agents that have a direct toxic effect on living cells, a cell lysing detergent Triton-X-100 (Triton) and FeCl₃, a catalyst generating

Figure 5. Sterile inflammation induced by Triton or FeCl₃ injure draining lymphatics and cause the formation of lymph clots that completely occlude collector drainage. A. Schematics of experimental design. Intradermal injection of 10% Triton-X-100 or FeCl₃ was followed by intravenous injection of fluorescently labeled fibrinogen, and mouse was fixed/perfused at 24 hours. **B-D.** Fluorescent dextran mixed with Triton-X-100 (TX100) was injected in the distal ear skin in two radially distinct locations that are drained by separate branches lymphatic collectors. **B.** Intravital microscopy of early time points after injection of dextran-TX100. From **Left** to **Right:** marking the collectors at 1 minute; 5 minutes after injection, leakage from the collecting vessels is visible; 10 minutes later, the extent of dextran diffusion from the leaky collectors mask their original drainage path. **C.** 24 hours after a mix of dextran-TX100 was injected, fluorescent dextran tracer re-injected i.d. is not drained by lymphatics. The chase with FITC-labeled fibrinogen leaked into the ear dermis and polymerized in the tissue, indicating disperse tissue injury but also within lymphatic collectors that were initially been draining the dextran-TX100 mix. Arrowheads in B and C mark the same collector locations. Fluorescent angiography performed 24 hours after i.d. injection revealed blood circulation deprived zones (**NC**-no circulation zones) in the skin where dextran-TX100 mix was injected. **D.** The whole-mount imagining of the skin collecting lymphatics fixed-perfused one day after the TX100 treatment. **Left:** Fluorescent fibrinogen that leaked from blood vessels polymerized within draining lymphatics, completely occluding their lumen. Insert represents a 5µm transverse optical section through an occluded lymphatic collector. **Middle.** The intracellular localization of CD31 is present in lymphatic draining control lateral ear side stains cell-cell junctions before the valve emptying into the clot-occluded lymphatic collector (arrowhead). In contrast, junctional staining is lost in the TX100- damaged collector, and instead, CD31 signal is evenly distributed across

injected dextran mixed with 1% detergent Triton-X-100 was drained initially by collecting lymphatics, to be leaked out of the lymphatic collector into the remote tissue only minutes later (**Fig. 5B**). Lymphangiography repeated on the next day showed that draining of cell lysis agent blocked the tissue drainage completely and instead lymphatic collectors were filled with continues lymph clotting (**Fig. 5C**). As expected, angiography performed day after intradermal injection of Triton showed that blood circulation was lost around the injection spots, confirming Triton in vivo universal toxicity and capability of blocking blood circulation. Optical sectioning of whole mount preparation of the injected skin revealed that fibrin clot filled completely lumen of the draining lymphatic, which lost the fine organization of cell-cell junctions (**Fig. 5D**). However, the Triton toxicity was limited to the collectors specifically draining detergent as afferent lymphatic draining control region but joined to the fibrin occluded collector vessels, but also blood capillaries surrounding occluded lymphatics, preserved their cellular organization. Already one day after the treatment surrounding tissue and fibrin-occluded lymphatics were populated by rounded inflammatory cells. Different mechanism of FeCl$_3$ toxicity that is dependent on free radical generation from H2O2 produced in mitochondria surprisingly lead to the same final effect, with blocked collector drainage and deposition of fibrin clots within lymphatic (**Fig. 5E**). In addition, similar to Triton X-100, intradermal injection of ferric chloride resulted in complete cessation of blood circulation around dermis injection sites. Fibrin clots filled completely lumen of lymphatics draining ferric chloride, which also lost its fine CD31-delinigthed junctional organization (**Fig. 5F**). Likewise Triton, ferric chloride toxicity was limited to draining lymphatic as lymphatics directly connected to a fibrin-occluded collector but draining lateral (control) skin and surrounding blood capillaries preserved their cellular arrangement. Also, a large number of rounded inflammatory cells infiltrated the dermis in the draining region and crowded within the fibrin of occluded lymphatics.

Specific decellularization of remote collectors leads to complete and long lasting clot formation and lumen occlusion

Injection of general toxins envisaged the importance of anti-clotting properties of the endothelium from lymphatic collectors. It also pictures ease and specificity with which they can be targeted, additionally proving that blocking of only a few lymphatic collectors ceases the drainage from the whole lymphatic tree. Including intact vessels draining the lateral side of the ear skin which are connected to the occluded lymphatic (**Fig. 5D and F**). This approach unspecifically exerts bystander toxicity to any cell type present at the site of injection. Also, toxins cannot be inactivated and instead they can freely diffuse outside the collectors potentially injuring cells in remote locations. Instead, photodynamic therapy (PDT) offers a solution to all these limitations. PDT is a combined physicochemical treatment where intradermally injected photosensitizer acts as proto-toxin, which is activated and destroyed with laser light at a defined location. This treatment assures that the toxicity of free radicals diffusing on short distances (up to 7 μm) will be strictly limited to collectors' associated cells[49]. Large, 100nm in diameter Visudyne® liposome enclose an active compound, a small molecular verteporfin, therefore their diffusion potential in the tissue was minimal. Practically, Visudyne® liposomes were either directly injected to the lymphatic collectors or retain in the skin interstitium. To avoid direct toxicity to the dermis that could result in enhanced trafficking of immune cells from the afferent injury site, the injection spots were painted black and covered with foil immediately after the injection only leaving the exposed collectors. We reached 98% of the reproducibility of the anti-lymphatic treatment by confirming phototoxic self-annihilation of Visudyne® within lymphatic collectors. This was done by imaging Visudyne® fluorescence before and after irradiation, which allowed us to eliminate mice with incompletely or poorly injected collectors. The routine anti-lymphatic treatment occluded all collectors draining peripheral dorsal skin within 24 hours after PDT with continues lymph clots (**Fig. 6B**). Likewise injection of directly-acting toxins, Triton or ferric chloride (**Fig. 5**), and in contrast to TF-stimulation (**Fig. 1-2**) or thrombomodulin blocking (**Fig. 3-4**), PDT always resulted in the formation of continuous intralymphatic fibrin clots in all vessels that drained photosensitizer (**Fig. 6B**). In contrast to directly-acting toxins, PDT resulted in much lower collateral damage to the tissue at the injection site that was manifested in minimal leakage of fluorescent plasma into a tissue (compare **Fig 5C and D with Fig. 6B**). Endothelial cell death deduced from degeneration of cellular junctions was specific to endothelial lining coming in direct contact with a photosensitizer, leaving afferent vessels draining lateral side of ear dermis intact (**Fig. 6D**). Basement membrane that supports endothelium and muscle cells of lymphatic collectors (**Fig. 6D**), remained as a scaffold

Figure 6. Specific decellularization of lymphatic collectors leads to complete and long-lasting lumen occlusion. A. Schematics of experimental design. Endothgelium was stripped from lymphatic collectors with a photodynamic therapy (PDT). Specifically, intradermal (i.d.) injection of photosensitizer verteporfin Visudyne® was followed by collector imaging (verteporfin lymphangiography) and subsequent irradiation of dorsal ear skin. 20-30 min after PDT, fluorescently labeled fibrinogen was injected intravenously, and ear lymphatics were imaged the following day. The mouse was fixed/perfused on the indicated day for whole mount imaging. **B.** Intravital microscopy, C-F-confocal imaging of whole-mount skin preparations. **B. Left:** Saline injection and repeated lymphangiography had no effect on collector perfusion in the control ear. **Middle:** PDT leads to occlusion of lymphatic collectors, which stop draining i.d. injected fluorescent dextran. **Right:** The same collector networks become occluded with

insoluble fibrin that leaked from blood vessels. **C-E.** Whole-mount imaging. **Left:** VE-cadherin is localized at cell-cell-junctions in regular lymphatic collectors of the ear skin. **Middle, Right:** VE-cadherin organization is lost in vessels that drained photosensitizer (**Vert**), while in the same ear, control lymphatic (**Ctrl**) draining lateral to the Visudyne® draining collectors or neighboring blood vessel (5 μm away) were not affected by irradiation. **D. Left:** Lymphatic endothelial cells (**VE-Cad**- VE-cadherin) were enclosed within the basement membrane (stained for laminin). P-basement membrane imprints of collecting vessel pericytes. **Middle:** Morphologically unaffected, cell-deprived basement membrane tubes- ´ghost vessels´- one day after PDT. BM scaffold was preserved in PDT-decellularized collectors. **Right:** Ghost vessels were filled with fibrin clots that blocked the whole lymphatic lumen. Insert shows 5μm cross-section of the fibrin-occluded collector. Frequently, basement membrane particles could be found trapped within a clot (arrowhead). **E.** In addition to intralymphatic lymph clotting, ghost vessels become infiltrated with TGFβ⁺ leukocytes that densely pack within the collector. **F.** From day 4 to 7 fibrin clots are cleared and partially replaced with tissue deposits containing basement membrane elements of laminin that are subsequently removed from vessel lumen(day 7 to day 10). The intensity of CD31 was normalized to its signal level in the lymphatics draining control region. The intensity of lymphatic fibrin deposits was normalized to the signal level of clots at the sites of injection (*). Scale bar: B, 250μm, C, D, E-100μm, F-25μm.

where lymphatic clots formed occluding the lumen of "ghost vessels" (**Fig. 6D**), named after similar blood vessel-derived structures that were described earlier by Inai[50]. Even though the basement membrane of collecting lymphatics remained intact, some degeneration occurred as BM particles could be found trapped within the fibrin clots (**Fig. 6D**, insert). Fibrin-occluded lymphatics were densely infiltrated by rounded neutrophil-like immune cells from day two after PDT. Leukocyte clusters persisted at the cone of advancing endothelial cells that regenerated ghost vessel (**Supplementary Fig. 3**), possibly providing directional and stimulating cues by the release of, e.g. TGFβ (**Fig. 6E**) to re-growing endothelium[51]. In contrast to fibrin deposits within ghost vessels, which began to clear from day 4 onward, massive leukocyte infiltration persisted throughout the regeneration period of lymphatics even though (**Fig. 6E**). Fibrin deposits were eventually either cleared or replaced with abnormal non-sheet-like masses of basement membrane matrix, containing laminin,(**Fig. 6F**), collagen IV, collagen III and tenascin C (not shown). Basement membrane deposits eventually evanesced from vessels approximately by day 9, which coincides with lymphatics re-gaining their drainage functionality ([49] and **Fig. 10b**). Interestingly, similar intralymphatic matrix deposits, composed of collagen type I and IV we found within peritumoral collecting lymphatics in implanted dermal B16-F10 melanoma, which was paralleled by the abnormal, discontinued organization of lymphatic endothelial cells. (**Supplementary Fig. 1**).

Endothelial cell death precede lymph clotting and is independent on tissue factor

We could not find even a theoretical mechanism explaining why killing of lymphatic endothelial cells but not its basement membrane scaffold should lead to occlusion of collectors without implication of secondary mechanism, namely lymph clotting. This also suggests that the primary function of lymphatic collectors could be the control of lymph fluid state.

Live imaging of skin collector vessel endothelium expressing Tomato-fluorescent protein under Prox1 promotor, with basement membrane stained for collagen IV showed that irradiated cells draining proto-toxin Visudyne® died between 1 and 3 hours after PDT (**Supplementary video 1, Fig. 7A**). Vertical afferent lymphatic collector served as internal control for imaging-dependent bleaching and phototoxicity and showed that only prior laser irradiation of drained photosensitizer but not subsequent fluorescence imaging evoke death of lymphatic endothelium. As expected, there was no

Video 1. Lymphatic endothelium died off within two hours after photodynamic therapy
The video presents a higher temporal resolution of events shown in Figure 7A. Morphology of major collectors was identified with intravital staining for basement membrane (collagen IV) and co-expression of ProxTomato protein. For clarity, collagen IV staining is not shown on the video (see Fig. 7A). As images were taken every one minute, Tomato-positive cells death appears as sudden ´switching off´ (begins at the left side of the horizontal lymphatic) or gradual dimming (right side of the horizontal lymphatic), either due to local conditions for protein diffusion or the level of injury. Some budding (the indicator of apoptosis) was observed on endothelium treated with photodynamic therapy (PDT, left compartment of the horizontal vessel), while most cells die by necrosis. Cells dying by apoptosis do not lose their intracellular fluorescence intensity, and instead, their cytoplasmic proteins are compartmentalized into apoptotic bodies dispersing by Brownian movements. Cells dying by autophagy accumulate their content in lysosomes, which initially become brighter than the surrounding cell and do not spread by Brownian movement. Possible some cells underwent apoptosis or autophagy at the left end of the horizontal vessel. Instead, cell dying by necrosis at various speed diffuse content of its cytoplasm to the surrounding, which can be seen as dimming or switching off, depending on the rate of the diffusion (compare with Video 3). The imaging began 10 minutes after PDT. First cells started dying 50 minutes after PDT, and most cells within lymphatics were dead 2 hours later. The real-life duration of the video is 5 hours (timer jamming during video play are due to buggy Leica software export module). The video frame rate is 20 fps.

quenching of intracellular Tomato proteins during imaging with low-power mercury lamp used in our fluorescence imaging setup[52]. Lymphatics expressed Tomato fluorescent protein in their cytoplasm that either should diffuse out of the necrotic cell or be compartmentalized into fluorescent apoptotic or autophagosomes bodies during programmed cell death as it is shown in **Supplementary video 2**.

We showed before that cell killing with PDT occurs by necrosis as cells become permeable to propidium iodide

Video 2. Concurrent necrosis and apoptosis of B16-F10 cells grown for one week in the mouse ear. Single cell divided but the two daughter cells die by apoptosis (top cell breaks into small apoptotic bodies which intensity is not different to the mother cell) and necrosis (bottom cell "explode," the GFP fluorescence diffuse out in 1-2 frames of the 15 fps movie). The color gradient, from high-contrast white to green, representing the weakest signal was chosen for the clarity of the visualization. The real-life duration of the video is 2 hours. The video frame rate is 15 fps.

the majority of endothelial cells treated with PDT diffuse their cytoplasmic proteins, the more informative indicative of the final stage of necrotic cell death (**Suppl video 3**). Despite that collector's endothelium dies off within 2.5 hours after PDT vessel occlusion started not earlier than 3 hours after PDT (**Fig. 7B**), which is in agreement with

Necrotic death of lymphatic endothelial cells at the level of the valve 2 hours after photodynamic therapy. Propidium iodide, a membrane impermeable DNA-binding agent labels nuclei of necrotic cells. The real-life duration of the video is 8 minutes. The video frame rate is 4 fps.

our previous results[49]. The cessation of dextran drainage between 3 and 5 hours after PDT correlated with increased deposition of fibrin within collectors that reached its maximum 7 hours after PDT. As compared to blood vessel occlusion, the process that is completed within minutes after the injury, occlusion of lymphatic collector after PDT-induced decellularization was a slow process that took at least an hour and began with fibrin deposition on the wall of decellularized lymphatic and continued toward the center of the vessels (**Suppl video 4**).

within 1.5 hours after the treatment[49]. Here we show that

In contrast to lymph clotting provoked by cytokines-induced TF-expression, intralymphatic clotting after PDT-decellularization could not be prevented with TF blocking

Video 4. Fibrin deposition on the wall of collecting lymphatic 2 hours after treatment with PDT
Imaging that started 2 hours after PDT and 1.5 hours after intravenous injection of FITC-fibrinogen was continued for 2 hours with images taken every minute. Microinjuries that are the effect of surgical exposition of dorsal dermis lead cased generalized leakage of plasma from vessels leading to an increase in fibrinogen fluorescence outside blood vessels. Immediately after PDT, mouse ear dorsal skin was exposed, and dermis was stained with collagen IV (not shown) to identify draining lymphatic vessels based on their characteristic morphology. The real-life duration of the video is 2 hours. The video frame rate is 15 fps.

antibodies (**Fig. 7C-D**). Also, TF-blocking did not inhibit infiltration of leukocytes into decellularized lymphatics, despite the fact that antibody were present in the tissue two days after the treatment. Most importantly, we confirmed our previous observation that there is a temporal gap between endothelial cell death and lymphatic occlusion, which indicated that at least during this lag period decellularized lymphatics were able to drain fluid without a presence of endothelial cells.

Massive infiltration of antigen presenting cells and T-cells begin after lymphatic occlusion and persist until their regeneration

Cessation of drainage after lymphatic decellularization is directly associated with the formation of intralymphatic clots of fibrin inside collectors but also massive infiltration of leukocytes (**Fig. 5E**). Here we asked if the latter phenomena could participate in the occlusion of lymphatics. In addition, we wanted to know what cell types are represented in the immunological clusters that form within lymphatics.

In contrast to fast infiltration of leukocytes into ghost lymphatics after intradermal injection of directly toxic compounds, Triton or ferric chloride, milder decellularization of collectors with PDT resulted in 24-hour lag phase and during that time leucocyte presence build up only around fibrin occluded lymphatics (**Fig. 6A**). Surprisingly, labeling of muscle cells smooth muscle actin with mouse monoclonal antibody revealed that intralymphatic clots could be directly stained with detection anti-mouse IgG antibody indicating that mouse

Figure 8. Massive infiltration of antigen presenting cells and T-cells into ghost vessels follows intravascular lymph clotting.
A. Time course of leukocyte (CD45+ cell) infiltration into ghost vessels (as visualized by staining of laminin of basement membrane). Leukocyte accumulation within ghost vessels cannot be distinguished from that of control lymphatics for the first 24 hours after vessel decellularization, although leukocyte build-up in peri-lymphatic tissue is already apparent at 6 hours after PDT. A dramatic change in leukocyte accumulation within lymphatics occurs between 24 and 48 hours after PDT-dependent decellularization - lymphatics become densely filled with leukocytes making this leukocyte manifestation an identifier for decellularized vessels. Arrowheads point to intralymphatic protein clusters visualized with anti-mouse IgG antibody used to reveal mouse anti-αSMA staining. Arrows point to leukocytes clusters within ghost vessel. **B.** Dense leukocyte accumulation within lymphatic vessels persists for the whole regeneration time of lymphatic, observed up to 10 days. The majority of cells within lymphatics are MHC class II-positive antigen presenting cells. While Gr1-positive neutrophils and monocytes remained in the surrounding dermis. **C.** **2 days** after decellularization. Single imaging field showing F4/80+ neutrophils and macrophages infiltrating dermis-surrounding collectors. However, they almost exclusively remain in the tissue and do not invade ghost vessels. **4 days** after decellularization. Single imaging field is showing that CD3ε+-T cells are the other abundant cell type that swarms ghost vessels by 4 days after decellularization. Arrowheads point to the border of a lymphatic collector marked by a residual sheet of fibrin, which delineates characteristic uneven diameter along the length morphology of lymphatic collecting vessels. Scale bar: 50μm.

IgGs derived from blood plasma are also trapped within lymph clots. Also, anti-mouse IgG staining also revealed that only a few IgG-expressing cells were present in the tissue of PDT-treated lymphatics, which was confirmed with anti B220 staining (not shown). The delayed infiltration of collectors is probably due to the preservation of afferent initial lymphatics and injection site, which in case of Triton or ferric chloride injection, connect with collectors

Figure 9. Heparin sustains lymphatic drainage in the deendothelized vessels. With inhibited clotting, decellularized lymphatic ghost vessels drain antigens and immune cells to the lymph node. **A.** Schematics of experimental design. Intradermal (i.d.) injection of Visudyne® mixed with 0.5 IU of heparin or saline is followed by collector imaging (verteporfin lymphangiography). Subsequently, the dorsal ear is irradiated with a 692nm laser (photodynamic therapy PDT). Thirty min later fluorescently labeled fibrinogen was injected intravenously (i.v.). Within the hour, and 6 hours after PDT, the same location in the ear skin was re-injected i.d. with 0.5 IU of heparin in 2.5 μl saline or saline alone. Eighteen hours later, fibrin deposits in the ear were imaged. Before fix-perfusion or at indicated time point functionality of ear lymphatics were assayed with fluorescent lymphangiography using intradermal dextran injection. **B.** Live imaging (live), **Top**: Heparin administration prevented intralymphatic clot formation along decellularized lymphatics. **Bottom**, lymphangiography: In the absence of intralymphatic clots, the decellularized lymphatics were able to drain fluorescent dextran. However, ghost vessels were permeable and leaked the tracer into the dermis. Whole-mount imaging (fixed). Decellularized lymphatics can take up large particles, demonstrated here with autofluorescent erythrocytes. By repeating injections of heparin, erythrocytes from non-coagulated blood enter the non-occluded, decellularized ghost vessels. **C.** Administration of two consecutive doses of heparin on the day of lymphatic decellularization was sufficient to maintain ghost vessel patency and drainage as seen at 2, and 10 minutes after i.d. dextran injection. Their leaky state persisted for 12 days. Arrows point to leaky lymphatic vessels. **D. Top**: Lymphatic function was assayed with fluorescence lymphangiography before injection of EGFP-splenocytes into the ear skin. Functional, PDT-decellularized lymphatic collectors remain patent with concomitant heparin injections but leaky. **Bottom**: Representative flow cytometry plots of EGFP splenocytes in the draining lymph nodes (DLN) and non-draining lymph nodes (NDLN) in control, and in DLN in PDT, PDT-heparin groups 24 hours after i.d. injection. Summary plot of flow cytometry EGFP+ cell counts. The red triangles in PDT-heparin group correspond to ears where heparin injection preserved dextran drainage as determined with fluorescent lymphangiography done prior splenocytes injection (D, top). Intensities of Gr1 and F4/80 were normalized to signal level of interstitial cells positive for these receptors. Scale bar: B-live, C, D-200 μm, B-whole-mount-50μm,

as one necrotic zone (**Fig. 5**). This also indicated that it is fibrin clotting and not leukocyte accumulation within decellularized lymphatic directly followed endothelial cell death and was accurately correlated with lymphatic occlusion. Interestingly, the antigen presenting cells (**Fig. 8B-C**) and T cells consist of the vast majority of cells that infiltrated ghost vessels while Gr1-positive neutrophils or monocytes and F4/80-positive macrophages and monocytes only populated ghost vessels-surrounding dermis (**Fig. 8C**). Antigen-presenting cells that populated ghost vessels expressed CD11c (**Supplementary Fig. 4**),

the marker of dendritic cells[53].

The presence of endothelium on collectors is not necessary for fluid drainage and cell trafficking
Decellularization of collectors leaves an intact tube of basement membrane that is initially filled with impermeable fibrin clots to be later replaced by the basement-membrane-like matrix (**Fig. 6**). Since these ghost vessels were capable for at least short time drainage after decellularization, we asked whether lymphatic endothelium is at all needed for fluid drainage and traffic leukocytes to the lymph nodes. To do that, we tried to block lymph clotting by intradermal

injection of heparin. This procedure was successful in 25% cases, as determined by the absence of fluorescence fibrin deposits (**Fig. 9B, live**). Without intravascular lymph clots decellularized lymphatics were able to drain dextran, however, their drainage was dysfunctional as they leaked collected fluid along their path. Nonetheless, even though not efficiently, lymphatics in the absence of endothelial lining are capable of delivering macromolecules (e.g., antigens) to the draining lymph node. Furthermore, in the absence of endothelial lining and intralymphatic clots, remote segments of ghost vessels could be filled with erythrocytes, large particles that in contrast to fluid did not leak outside the basement membrane tube even 48 hours after injection (Fig. 9B, fixed). This indicates that endothelium is not necessary for cell passage to the draining lymph node. Interestingly, once ghost vessels were protected from the occlusion for 24 hours after the PDT, they stayed patent. Their draining state could be verified with lymphangiography even 12 days after PDT when all patent vessels drained dextran, but only collectors that recover endothelial lining were not permeable to the fluorescent marker already few minutes after the injection (**Fig. 9C**). Most importantly, decellularized collectors whenever they remained patent and drained fluorescent dextran were also capable of trafficking leukocytes, most importantly dendritic cells, to the draining lymph node (**Fig. 9D**), proving that presence of endothelial lining is not necessary for this process. At the same time, these results prove that occlusion of collectors with clotted lymph is sufficient to completely block the drainage of macromolecules (e.g., antigens) and trafficking of any kind of cells from the tissue to the draining lymph node. Additionally, skin edema that develops one day after PDT was resolved on day 5 before any functional regeneration of lymphatics took place (Supplementary Fig. %). This is however in agreement with early observations, wherein the absence of persistent inflammation lymphatic occlusion alone does not produce lymphedema[54].

Lymphatic occlusion is sufficient to hide allograft from the detection of the immune system

Due to the potent and acute cytotoxic response and little effect of the immunosuppression on allograft tolerance, skin transplantations confined to autografting[55]. However, cutaneous immunity has one significant vulnerability as its responsiveness depends on functional lymphatic system[56] that connects the drained skin with secondary lymphoid organ[57]. Allografts are accepted indefinitely when transplanted to a location that could not drain to the lymph nodes because of induction of immune ignorance rather than tolerance[57, 58]. Since we understood the occlusion mechanism and the kinetics of lymphatic regeneration, next, we planned to test the efficacy of the temporal lymphatic blockage on the prolongation of subcutaneous allograft acceptance. To do that we established highly reproducible and sensitive subcutaneous heart transplant model[59]. In contrast to skin-over-skin transplant assays, transplantation of self-contracting cardiac tissue provides a natural rejection parameter that can be visually assayed daily. Additionally, a pocket formed between cartilage

and dorsal skin completely protected the implant from drying and infection and provided blood supply from the uninjured dorsal dermis. This assured a high level of the initial vascularization of the transplants (over 95%, Fig. 10A), which is the most critical parameter in avoidance of artifacts like considering necrotic rejection as immunological rejection [60]. Transplanted under dorsal ear skin halves of the newborn mice hearts were vascularized within 5 days after implantation and started contraction that was monitored through the skin (**Supplementary video 5**).

Video 5, Contracting isograft of cardiac muscle under BALB/c skin, 9 days after transplantation.

Control isograft or isograft transplanted under the PDT-treated ear skin were accepted until the end of the experiment (**Fig 10B**). In contrast allografts, median rejection time was 8 days (**Fig. 10B**). The average graft survival was extended to 12 days when allografted hearts were implanted under PDT-treated skin. In addition, the rejection kinetics in control and PDT groups were different. While the control tissues were rejected across the 5 day period, the rejection in PDT group is almost binominal and occurred within one day. This could be explained by the high level of lymphatic regeneration homogeneity (**Fig. 10C**) but also the fact that ghost vessels before regeneration of lymphatics become tertiary lymphoid organs[61], with an accumulation of antigen presenting cells ready to be delivered to the draining lymph node (**Fig. 8**). Conceivably, as the time of vessels regeneration was delayed with anti-VEGFR3 therapy (**Fig. 10C**), the time of allograft acceptance was almost doubled from the original 6 to 15 days. Interestingly, this value is better than presented with the same assay results on the effect of commercial cyclosporine (Sandimmune) treatment on allograft rejection that occurred after 9 days in control and 13days cyclosporine-treated group[62].

Alloantigen-specific antibody that develops after the tissue implantation is generally considered not relevant for an acute cytotoxic response. Yet, their level and subtype constitute significant parameter in probing immune ignorance as the production of allo-specific antibody,

Figure 10. Lymphatic occlusion hides antigens and prevent rejection of skin allograft. Murine embryonic contractile cardiac tissue was transplanted under ear dermis of the fully immunocompetent mouse with or without lymphatic-specific photodynamic therapy (PDT) and observed for functional muscle contraction, plotted as % graft acceptance rate vs. number of days of graft survival (**A, B**). **A.** Isografts from control group (n=6, 5 censored) and PDT group (n=6, 6 censored) continued contracting until the planned termination of the experiment (31 days) where lymphatic collector decellularization with PDT had no effect on isograft acceptance. (Mantel-Cox log-rank test (p<0.32). All implanted hear fragments resume contraction after implantation. **B.** The median survival time of allografts transplanted under control mouse dermis was 8 days (n=17 mice, 16 rejected, 1 censored). When allografts were implanted under immuno-priviliged ear dermis with PDT-occluded lymphatics, the kinetics of allograft rejection was uniform, and graft median acceptance was prolonged to 12 days (n=18 mice, 14 rejected, 4 censored). This median acceptance time of the allogeneic transplant grafted under PDT-decellularized lymphatics was prolonged to 15 days (Mantel-Cox log-rank test (p<0.0001) with adjuvant anti-lymphangiogenic therapy with intraperitoneal administration of anti-VEGFR3 antibody (PDT αVEGFR3 group, n=11 mice, 10 rejected, 1 censored). All censored cases in allograft groups were due to failure to resume contraction during the first 5 days after the implantation. **C. Lymphangiography**, quantification. 7 out of 9 ears harboring subcutaneous implant resumed lymphatic drainage 11 days after treatment in PDT group. In contrast, mice receiving adjuvant αVEGFR3 antibodies after PDT-induced lymphatic decellularization had only 2 out of 10 ears that resumed drainage (p=0.023, Fisher exact test). Representative

and antibody class switching reflects the availability of alloantigens in the lymph node[63]. The seven-fold relative increase of the earliest released IgM alloantibody was the highest between all tested isotypes (Fig. 10C) indicating that anti-lymphatic (PDT) therapy reduced the increase of allospecific antibody to 1.4 fold (2.4-times), with further reduction to the basal level (0.4 fold increase) was measured when anti-lymphatic therapy (PDT) was followed by lymphatic regeneration delay with αVEGFR3 therapy. Even though the level of antibody in PDT and PDT-αVEGFR3-treated groups were not different to the respective basal levels, the pattern of antibody decline with middle values after only PDT and almost basal after PDT+αVEGFR3 was reproduced for every subtype (five curves not different, p<0.05). This means that rather than the development of immune tolerance, the immune reaction was only delayed and that alloantigens that remain outside the reach of the lymph node did not lead to T-cell tolerance. Instead, these alloantigens are 'ignored,' and the alloreactive T cells remain functionally intact and can be engaged when tissue clearance is restored.

Discussion

Here we characterize anti-clotting properties of the lymphatic collecting vessels and their application in the on-demand cessation of antigen drainage and trafficking of antigen presenting cell. This leads to the creation of subcutaneous immune-privileged zones where allografts can be protected from immune-recognition without immunosuppression. We show that fluid drainage and immune cell trafficking entirely depend on lymphatic vessel ability to sustain lymph liquidity.

Physiological function-mechanisms of intralymphatic clotting

Regardless of the method of lymph clotting induction, intravascular lymph clots interfered with essential lymphatic functions, fluid and macromolecule evacuation from the drained area of the skin. Intralymphatic clots were detected by copolymerization of fluorescently labeled fibrinogen. Because FITC-fibrinogen was injected intravenously, first it had to leak with other plasma proteins to the tissue (at the site of prior intradermal injections). Later these proteins were collected by lymphatics and drained as naturally formed lymph. Therefore the fluorescent labeling of intralymphatic clots reflected the natural process of lymph coagulation.

In contrast to selective induction of pro-hemostatic TF expression that resulted in discrete and sparse lymph clots deposition within collecting lymphatics (**Fig. 1-2**), inhibition of constitutively expressed thrombomodulin resulted in widespread lymph clotting inside efferent vessels (**Fig. 3B and 4B,C**). These lymph clots formed within intact lymphatic intima were cleared within subsequent 16 hours, therefore, their physiological or

therapeutic relevance is limited to extemporary, e.g., inhibition of bacterial spread in early acute inflammation, as previously reported[64-66]. Similar to thrombomodulin inhibition, decellularization of lymphatic intima lead to massive and continuous lymphatic occlusion independent on LEC expression profile or their location within collector, leaving ´ghost vessels´ composed of acellular basement membrane filled with lymph clots (**Fig. 5-6**). Experiments with injection of necrotizing compounds, i.e. TritonX and FeCl$_3$ (**Fig. 5**) aimed to confirm previous observation where intradermally administrated turpentine or FeCl$_3$[64,66] lead to cessation of lymphatic drainage by intralymphatic lymph clotting (referred as ´thrombosis´, experiments reviewed by Drinker and Field[14]).

Both, TritonX and ferric chloride exerted toxicity at the site of injection but also completely blocked the skin drainage and induced lymph clotting in the lymphatics located remotely to the site of intradermal injection. The same effect of lymphatic occlusion but without adverse skin, necrosis was achieved with PDT-induced lymphatic decellularization (**Fig. 6-10**). Due to the high specificity of anti-lymphatic treatment and the long-lasting (9 days) drainage occlusion, we used this method to study the effects of intravascular lymph clotting on lymphatic physiology and local immune responses.

Despite the type of lymphatic treatment, lymph clotting was an endpoint that preceded interference or complete blockage of fluid drainage. Even though leukocytes involvement in fibrin polymerization and maturation within lymphatics could not be excluded; the initial lymph coagulation occurred before leukocytes infiltration (**Fig. 2 and 8**). Therefore, in one way or another lymph clotting was dependent on lymphatic endothelium that either expressed TF after stimulation lost anti-hemostatic properties after thrombomodulin blocking or was destroyed by detergent lysis (Triton-X-100), exposure to free-radicals generated by FeCl$_3$ or free-radicals generated by light-activated verteporfin (i.e., lymphatic-specific PDT). However, the duration of lymphatic occlusion varies significantly between the metabolic and noxious methods of lymph clotting, from less than 22 hours with preserved intact endothelium to 9 days[49], when collectors were decellularized. Initial lymph clotting could be activated by dying cells releasing pro-thrombotic negatively charged RNA and polyphosphates that can activate factor XII of the contact-dependent (intrinsic) coagulation pathway[45]. Intrinsic pathway can be also continuously activated by the constant exposure of lymph to the unmasked basement membrane collagens ([33] and **Fig. 6C-D**), which in the absence of endothelial membrane-bound antithrombotic thrombomodulin([19] and Fig. 1A) can lead to recurrent activation of lymph coagulation even when the initial clot is cleaved 4-5 days after PDT-driven decellularization of

lymphatics (**Fig. 6F**). Stability of intralymphatic clots is additionally enhanced by the loss of the endothelium that is a source of tissue plasminogen activators[21], which production is enhanced after pro-thrombotic stimulation of endothelium (Fig. 3D). Therefore, restoration of lymphatic intima should be the critical factor in stable preservation of collector patency. This conclusion is in agreement with our subsequent finding that lymph clotting but not the loss of endothelial lining was a direct cause for lymphatic occlusion to fluid and cells. This is indicated by a delayed block of drainage that occurred hours after endothelial death (**Fig. 7**), and most notably by sustained fluid drainage and cell trafficking through PDT-decellularized collectors when fibrin deposition was inhibited with heparin (**Fig. 9**). Even though decellularized collecting lymphatics were leaky to drained dextran, this experiments indicated that endothelial lining is not indispensable for the most affirmed functions of lymphatics, the fluid drainage, and cell trafficking and instead lymphatic endothelium is primarily needed to support collector's patency.

Intravascular lymph clots delay of allograft rejection -therapeutic applications

The lack of conventional lymphatic drainage is a characteristic feature shared between passive immune ignorance[57] and immune privilege at sites like placenta, cheek pouch, cornea or central nervous system[67-69]. Furthermore, it was shown that surgical separation of draining lymphatics blinds the draining lymph nodes to antigens residing within the blocked area and prevent the development of adaptive immune response against allograft at least for the time alternative lymphatic routes developed[70, 71]. Due to extensive and traumatic surgery, these experiments lack translational potential. Instead, they provided a proof of concept where elimination of antigen drainage path leads to the formation of immune privilege zone where foreign antigens remain ignored by adaptive immunity. Long-lasting occlusion of lymphatic collector that follows specific eradication of lymphatic intima allowed us to mimic the effect of mechanical laceration of the skin and prove the therapeutic applicability of the anti-hemostatic properties of lymphatic endothelium. Instead of skin transplant, where rejection is defined by subjective parameters[72], we used sensitive cardiac graft where the immune rejection is manifested by the loss of spontaneous contractile function[59]. Indeed, the rejection of allografts but also the development of allo-specific antibodies was delayed after PDT-dependent decellularization of collectors and correlated with drainage recovery from the skin surrounding the graft (Fig. 10). Importantly, the time of graft acceptance was doubled as the immune response was delayed when lymphatic regeneration was inhibited with VEGFR3 blocking antibodies. Possibility to further prolong allograft hiding from the immune-recognition with anti-lymphangiogenic therapy indicates that there are still opportunities for further enhancements in the adjuvant therapies, e.g., by reinforcing clotted lymph with matrix-bound protease inhibitors[73]. Interestingly, in the two combined relatively non-invasive treatments, lymphatic

decellularization with PDT and subsequent inhibition of lymphatic regeneration with anti-VEGFR3 antibody, had a stronger effect on rejection inhibition (delay by 47%) than immunosuppressant cyclosporine in a form of clinically-approved Sandimmun® (delay by 30%), when tested in cardiac allograft model[62]. However, it is important to appreciate the difference between these treatments, while lymphatic occlusion leads to immunological ignorance by hiding tissue from immune recognition in draining lymphatics, cyclosporine suppresses already developing an immune response.

Anti-clotting function of lymphatics in health and disease

We described the overlooked function of lymphatic vessels that might have significant consequences in various pathologies and therapies that until now could not be adequately appreciated. In homeostasis anti-hemostatic mechanisms helps sustain lymph as a liquid but during the acute inflammation, the protein-rich exudate that leaves blood vessels does not enter lymphatics, helping to circumscribe the infection from draining to the efferent vessels and eventually bloodstream, reviewed by Menkin[74] and Drinker[14]. This phenomenon of ´fixation´ of bacteria, protein, and particles to the site of early inflammation were attributed to the mechanical obstruction of lymphatics with fibrin leaking from inflamed or injured blood vessels. Unfortunately, as it could explain, e.g. why acute lymphangitis, an infection of lymphatic collectors is predominantly caused by plasmin-activating positive group A streptococci bacteria[75] the research on in situ lymph clots was not further studied[5]. On the other hand, the ability of dysfunction of lymphatics to sustain non-clotted lymph might contribute to their pathologies with idiopathic or confound origin. Surprisingly, even in case of thoroughly studied lymphedema, all causative factors are not known as lymphatic occlusion is a necessary but still insufficient factor to induce sustained lymphedema in animal models[22, 76, 77]. Also, lymph clots within lymphatics around the granuloma that form after worm death during the pathogenesis of filarial lymphedema[24] intuitively carry a notion that lymph clotting and inflammation might be important priming factors of the disease. Filaria-induced lymphedema develops after repeated instances of worm deaths and bacterial lymphangitis that additionally lead to lymphatic endothelium injury and fibrotic remodeling of lymphatic collectors[78]. Along these lines, our results indicated that inflammatory factors-stimulated lymphatic occlusion is transient and quickly resolved within lymphatic vessels, while injury to lymphatic endothelial lining is sufficient for prolonging occlusion of the collector. But even after PDT-induced lymphatic decellularization, ghost vessel eventually regenerated instead of becoming fibrotic[49]. PDT-decellularization is a specific and sterile anti-lymphatic treatment while trauma combined with infectious inflammation might produce long-lasting intralymphatic clot remodeling and permanent vessels occlusion with collagenous fibrosis, elements of which we could observe in lymphatics regenerating after PDT (Fig 6F). Also, anti-hemostatic properties of lymphatics should be the primary parameter that requires

consideration before designing lymphatic implants, e.g., artificial collectors lympho-venous shunts or lymphatic collateral neovessels[79] as they must anchor functional anti-hemostatic mechanism in order to canalize the edematous tissue permanently. Because until now, the anti-hemostatic property of lymphatic has not been yet fully appreciated, it is possible that lymph clotting and subsequent fibrosis is an underestimated complication unwittingly hampering lymphedema treatment. For example, unpredictable clotting and fibrinolysis cycles could explain the fact that most silicon tubes implanted in lymphedema patients did not drain the fluid along their lumen even though it did nor undergo fibrosis and remained patent[80].

The active regulation of lymphatic drainage might also affect tumor metastasis. Entrapped tumors or associated cells might activate fibrinolytic mechanisms and use residual fibrin scaffold to enhance their migration within the lymphatic system. This scenario is supported by experiments where depletion of fibrinogen inhibits lymphatic metastasis but has no effect on primary tumor growth[81]. Contrarily, completely occluded lymphatics might stop the spread of metastatic cells, likely the mechanism of PDT treatment that blocked the metastasis spread via peri-tumoral lymphatics [82]. In this situation lymphatics, control over lymph hemostasis is a potential new avenue for the research that could, e.g. aim at reinforcement of fibrin or local inhibition of fibrinolysis[73] in order to prolong a block cell dissipation along lymphatic collectors. Strengthening of intralymphatic clot resilience could also be used to delay further the regeneration of lymphatics occluded with PDT and by this extend the time subcutaneous allografts are masked and ignored by the immune system. Accessibility of the dermal lymphatics and low-risk subcutaneous surgery might permit therapeutic prosthetic transplantation of small hormone-producing various tissue fragments or cells, like Langerhans islets [83].

Here we identified anti-coagulatory properties of lymphatic collecting vessels and demonstrated their permissive influence on essential lymphatic functions, i.e., fluid drainage and cell trafficking. Interference with these properties lead to a various level of lymphatics blockage by the clotted lymph, otherwise drained in as a fluid by collecting vessels. Decellularization of lymphatic vessels resulted in complete loss of anti-coagulatory characteristics and long-lasting intralymphatic occlusion. In the absence of endothelium, the anti-coagulatory phenotype of lymphatic vessels, as well as their drainage, could be rescued with the injection of heparin, indicating a fundamental impact of lymphatic anti-clotting properties on their primary function. Finally, we showed that intralymphatic occlusion correlated with the delay of allograft rejection and development of adaptive immune response, the potential alternative approach to chemical immunosuppression after allogeneic tissue transplantation.

Methods

Animal experiments

Animal experiments were performed at the EPFL (Lausanne, Switzerland), the University of Chicago and the Medical University of Warsaw (tail edema experiments). Procedures performed on animals were in strict accordance with the Swiss Animal Protection Act, the ordinance on animal protection and the ordinance on animal experimentation. We confirm that our Institutional Animal Care and Use Committee (IACUC), named Commission de Surveillance de l'Etat de Vaud (Permit Number: 2646 and 2687), specifically approved this study or in accordance with protocols approved by the Institutional Animal Care and Use Committee at EPFL (permit number 72414). Procedures performed at the University of Chicago were performed according to rules and protocols at the University of Chicago were performed according to the guidelines approved by the Ethics Committee of the Medical University of Warsaw. BALB/c female or C57 mice were purchased from Jackson Laboratories or Charles River, maintained and breed in a specific pathogen-free barrier facility and used between 6 to 10 weeks of age unless stated otherwise.

Anesthesia and hair removal

Three days before each experiment, ears were treated with depilation cream (Veet® Hair Removal Cream, Slough, UK) for 10 s followed by thorough rinsing with water. For PDT, mice were anesthetized with 2.5 % isofluorane (Rothacher GmbH, Bern, Switzerland) and kept under 1.5 % isoflurane for the duration of the experiment. Mouse core temperature was maintained at 37 °C throughout the experiment (DC Temperature Control System, FHC Inc., Bowdoin, MA). All intradermal injection in the dorsal mouse ear (0.5 µl) was done using a microsyringe (Hamilton, Reno, NV, USA) equipped with 33 G needle.

Photodynamic therapy (PDT) on the mouse ear

Mouse head was epilated under isoflurane anesthesia 24 h before the procedure. Ears were treated with epilation cream (Veet) briefly for 10 s at the end of the head epilation process, and mouse head was washed with plenty of water. The mouse was allowed to recover in a cage with food and water ad libitum. On the day of the experiment, a mouse was anesthetized with 2.5% isoflurane and kept under 1.5% of isoflurane for the duration of the experiment. 0.5 µl verteporfin in the form of liposomes (Visudyne®, Novartis Ophthalmics, Hettlingen, Switzerland) freshly reconstituted from the powder as previously described[49] was injected in the top of the ear with Hamilton syringe (Reno). Injection site of the ear was covered by aluminum foil and 1 min later, the ear was irradiated with non-thermal laser light (Biolitec) or 2W LED laser (Modulight) at 689 ± 2 nm delivered through an optical fiber containing a frontal light distributor with a lens (Medlight) with the irradiance of 50 mW/cm2, and light dose of 100 J/cm2. Light doses were adjusted with neutral density filters and measured with a calibrated Field-Master GS power meter (Coherent).

Decellularization of lymphatics with detergent or FeCl₃

5% Triton-X-100 (TX100) and FeCl₃ (Ferrum chloride) were dissolved in water and filtrated through the 0.22µm membrane. 0.5µl of TX100 or Ferrum chloride was injected in two adjacent spots at the top of the ear dorsal dermis and immediately after that FITC labeled fibrinogen was injected i.v.

In vivo labeling of fibrin

40 ml 10 mg/ml fibrinogen (SIGMA) dissolved in in PBS was reacted with 1.6 ml of 4 mg/ml FITC (ThermoFisher) for 1 hour and fibrinogen was dialyzed 4 times to 4L each time of PBS. After that fluorescent fibrinogen was aliquoted and stored at -80°C until used. After thawing 200 µl of labeled fibrinogen was injected i.v. into mouse tail vain up to 15 to 30 minutes after treatment that was expected to induce intralymphatic coagulation (PDT, thrombin, cytokine injection).

Blocking thrombomodulin and TF expression on lymphatics

1 U/µl thrombin was reacted with 1 mM phenylmethylsulfonyl fluoride (PMSF, Sigma) for 2 hours and residual PMSF was removed on the Zeba™ desalting column (ThermoFisher Scientific). This treatment renders 85% of thrombin inactive as determined with the delayed fibrin clotting (from 45 seconds to 270 seconds).

Complete inactivation of thrombin was done by reacting of 50 µl of 1 U/µl thrombin with 1 mM p-amidinophenylmethylsulfonyl fluoride (p-APMSF, EMD Millipore Corp.[43]) µl of thrombin for 2 hours and residual PMSF was removed on the Zeba™ desalting column. 0.5µl of inactive thrombin or partially inactivated thrombin was injected intradermally alone or with 10ng/µl TNFα or 10vg/µl Il-1β in the ear top dorsal dermis.

Splenocytes trafficking into lymphatics

Splenocytes from BALB/c mouse expressing eGFP under ubiquitin promotor were isolated from the mouse spleen by grounding the spleen through the strained with 70µm pores. Red blood cells were lysed with RBC lysing solution (150 mM NH₄Cl and 10 mM NaHCO3) for 5 minutes, washed twice in DMEM and dissolved in Ringer's buffer buffered with 25 mM HEPES, pH 7.5. Cells were spun down for the last time, loaded to the Hamilton syringe with the pipette tip. After mounting 33G needle, 2.5 µl slurry was injected into the same location of the ear where verteporfin and heparin or Ringer was injected on the previous day.

Fluorescent intravital lymphangiography

Two hours after PDT and every 2-3 days 1 µl of TRITC-dextran (10 µg/ml) was injected in the location of initial verteporfin injection. Draining lymphatics were imaged with stereomicroscope after the ear was placed between two glass slides. For intravital lymphangiography, ventral skin with underlying cartilage was separated and removed from dorsal, PDT-treated skin and primary rabbit, anti-collagen IV antibody, was applied for 20 minutes. After brief washing with Ringer's buffer, secondary streptavidin-647 was applied for 5 minutes; tissue was washed and imaged using automated fluorescent stereomicroscope (M205 FA, Leica Microsystems) coupled to the sensitive color camera Leica DFC350 FX (Leica Microsystems). The following objectives have been used: Plan Apo 1x, NA 0.035; W.D. 60 or Plan Apo 2x, NA 0.07; W.D. 60 (Leica Microsystems).

Intracardiac perfusion and whole-mount staining of a mouse ear

Mice were sacrificed with CO2 and exsanguinated by intracardiac perfusion with 20 ml Ringer's buffer (supplemented with 10,000 IU/L heparin, 0.1% glucose, and 25 mM HEPES; pH 7.5, 330 mOsM) at a constant gravitational pressure of 120 mm Hg. Ringer's buffer was then changed to osmolarity-corrected zinc fixative (Zn fix) solution [26] (4.5mM CaCl2, 52 mM ZnCl2, 32 mM Zn(CF3COO)2, 2mM Triss, 38 mM glycine; pH 6.5, 340 mOsm/L) and ears were cut and placed in ice-cold Zn fix with 1% Triton x-100 for at least 24 h. After that, the ventral part of the skin was removed together with cartilage and muscles, and dorsal dermis was washed in TBS (140 mM NaCl, 25 mM Triss, pH 7.5) for 6 h, blocked with 0.5% casein in TBS (blocking solution) for 2 h, and incubated with anti-VE-cadherin, anti-Lyve-1, and biotinylated anti-collagen type IV antibodies (10 µg/ml) in blocking buffer for 24 h. After washing in TBS with 0.1% Tween 20, tissue was incubated with the appropriate secondary antibody (10 µg/ml) for another 24 h, washed in TBS and dehydrated with 70% and 100% ethanol before it was cleared with 2:1 benzyl benzoate/benzyl alcohol solution supplemented with 25 mg/ml propyl gallate (refractive index 1.56). The tissue was mounted on a glass slide and imaged using HC PL APO 20x, NA 0.70 or HCX PL APO 63x, NA 1.40 lenses of a Leica SP5 confocal microscope (Leica). Stacks of images were analyzed with Imaris 7.4 (Bitplane AG).

Transplant experiments

PDT was performed on ears on day 0 and on the next day newborn (1-2 days after birth) mice hearts from allogenic or syngeneic mice were cut in half and incubated in DMEM media. The incision was done on the ventral side of the mouse ear and spatula was inserted through the cartilage to the end of the dorsal, separating cartilage from dorsal ear skin. Inside the forming chamber, halve ear was inserted, and the ventral incision was sealed with surgical glue. 50 µl of the blood was collected on day 5 and 10, and isolated serum was frozen for further analysis. Heartbeat in mouse ear was monitored daily after short isoflurane anesthesia. Until the beating stopped when mice were perfused, and their ears were zinc-fixed for further analysis.

Detection of allo-specific IgM and IgG in grafted mice

Thymocytes from the allogenic background were isolated from 4 weeks old mice at 10x10⁶/ml, and 50µl of cells were mixed with 5µl of mouse serum isolated from mice bearing transplants on day 5 and 10. After washing, cells were incubated with appropriate isotype antibody or anti-IgM antibody, re-suspended for FACS buffer for acquisition in Beckman Coulter CyAn ADP flow cytometer.

Acknowledgement

The authors are grateful to S. Hirosue for editing the manuscript and advice, V. Triacca, E. Guc and J. Kilarska for their technical assistance and advice. The authors are grateful to the EPFL Bioimaging and Optics Platform and Histology Core facility for their technical assistance. Funding for this project was provided in part from the European Commission Framework Project 7 Angioscaff, and from the European Research Commission Advanced Grant LymphImmune, 323053 and Polish-Swiss Research Programme (PSPB-057/2010 to JG, WWK and MAS).

References

1. Gimbrone (1987). *Vascular endothelium: Nature's blood-compatible container*. Ann N Y Acad Sci
2. Rusznyák,&al. (1967). *Lymphatics and lymph circulation. Physiology and pathology*, Pergamon Press
3. Drinker,&al. (1933). *Lymphatics, lymph and tissue fluid*, The Williams & Wilkins Co
4. Miller,&al. (2000). *Haemostatic factors in human peripheral afferent lymph*. Thromb Haemost
5. Menkin (1960). *Biochemical mechanisms in inflammation*. Br Med J
6. Opie (1913). *Thrombosis and occlusion of lymphatics*. J Med Res
7. Copley,&al. (1942). *Bleeding time, lymph time, and clot resistance in men*. J Clin Invest
8. Fantl,&al. (1953). *Coagulation in lymph*. J Physiol
9. Mayanskii,&al. (1966). *A comparative study of the clotting power of the blood and lymph*. Bull Exp Biol Med
10. Le,&al. (1998). *Hemostatic factors in rabbit limb lymph: Relationship to mechanisms regulating extravascular coagulation*. Am J Physiol
11. Leak,&al. (2004). *Proteomic analysis of lymph*. Proteomics
12. Lippi,&al. (2012). *Hemostatic properties of the lymph: Relationships with occlusion and thrombosis*. Semin Thromb Hemost
13. Brinkman,&al. (1996). *Vessel wall-mediated activation of the blood coagulation system*. Vascular control hemost. Harwood Academic Publishers.
14. Drinker,&al. (1933). *Inflammation*. Lymphatics, lymph and tissue fluid. The Williams & Wilkins Co.
15. Aukland,&al. (1993). *Interstitial-lymphatic mechanisms in the control of extracellular fluid volume*. Physiol Rev
16. Wiig,&al. (2012). *Interstitial fluid and lymph formation and transport: Physiological regulation and roles in inflammation and cancer*. Physiol Rev
17. Engelmann,&al. (2013). *Thrombosis as an intravascular effector of innate immunity*. Nat Rev Immunol
18. Conway (2012). *Thrombomodulin and its role in inflammation*. Semin Immunopathol
19. Maruyama,&al. (1985). *Thrombomodulin is found on endothelium of arteries, veins, capillaries, and lymphatics, and on syncytiotrophoblast of human placenta*. J Cell Biol
20. Kirchhofer,&al. (1994). *Endothelial cells stimulated with tumor necrosis factor-alpha express varying amounts of tissue factor resulting in inhomogenous fibrin deposition in a native blood flow system. Effects of thrombin inhibitors*. J Clin Invest
21. Laschinger,&al. (1990). *Production of plasminogen activator and plasminogen activator inhibitor by bovine lymphatic endothelial cells: Modulation by TNF-alpha*. Thromb Res
22. Drinker,&al. (1933). *Lymph edema and elephantiasis*. Lymphatics, lymph and tissue fluid. The Williams & Wilkins Co.
23. Olszewski (2002). *De novo lymph node formation in chronic inflammation of the human leg*. Ann N Y Acad Sci
24. Case,&al. (1991). *Vascular abnormalities in experimental and human lymphatic filariasis*. Lymphology
25. Fader,&al. (1986). *Evolution of lymph thrombi in experimental brugia malayi infections: A scanning electron microscopic study*. Lymphology
26. Hara,&al. (2013). *Lymphoedema caused by idiopathic lymphatic thrombus*. J Plast Reconstr Aesthet Surg
27. Cluzan (2007). *Peripheral lymphedema treatment*. Phlebologie
28. Forster,&al. (2006). *Tissue factor and tumor: Clinical and laboratory aspects*. Clin Chim Acta
29. Ruf,&al. (2011). *Tissue factor and cell signalling in cancer progression and thrombosis*. J Thromb Haemost
30. Padera,&al. (2002). *Lymphatic metastasis in the absence of functional intratumor lymphatics*. Science
31. Idell (2003). *Coagulation, fibrinolysis, and fibrin deposition in acute lung injury*. Crit Care Med
32. Margaritescu (2015). *Cutaneous metastases of breast carcinoma*. Rare malignant skin tumors. Springer.
33. van der Meijden,&al. (2009). *Dual role of collagen in factor xii-dependent thrombus formation*. Blood
34. White-Adams,&al. (2010). *Laminin promotes coagulation and thrombus formation in a factor xii-dependent manner*. J Thromb Haemost
35. Bevilacqua,&al. (1984). *Interleukin 1 (IL-1) induces biosynthesis and cell surface expression of procoagulant activity in human vascular endothelial cells*. J Exp Med
36. Lupu,&al. (2005). *Tissue factor-dependent coagulation is preferentially up-regulated within arterial branching areas in a baboon model of escherichia coli sepsis*. Am J Pathol
37. Liu,&al. (2004). *Thrombin and tumor necrosis factor alpha synergistically stimulate tissue factor expression in human endothelial cells: Regulation through c-fos and c-jun*. J Biol Chem
38. Kilarski,&al. (2013). *Intravital immunofluorescence for visualizing the microcirculatory and immune microenvironments in the mouse ear dermis*. PLoS One
39. van Hinsbergh (2012). *Endothelium--role in regulation of coagulation and inflammation*. Semin Immunopathol
40. Jesty,&al. (2005). *Positive feedbacks of coagulation: Their role in threshold regulation*. Arterioscler Thromb Vasc Biol
41. Mackman (2009). *The role of tissue factor and factor viia in hemostasis*. Anesth Analg
42. Fuentes-Prior,&al. (2000). *Structural basis for the anticoagulant activity of the thrombin-thrombomodulin complex*. Nature
43. Laura,&al. (1980). *(p-amidinophenyl)methanesulfonyl fluoride, an irreversible inhibitor of serine proteases*. Biochemistry
44. Chen,&al. (2010). *Sterile inflammation: Sensing and reacting to damage*. Nat Rev Immunol
45. Esmon (2010). *Far from the heart: Counteracting coagulation*. Nat Med
46. Wu,&al. (1996). *Role of endothelium in thrombosis and hemostasis*. Annu Rev Med
47. Egorina,&al. (2008). *Granulocytes do not express but acquire monocyte-derived tissue factor in whole blood: Evidence for a direct transfer*. Blood
48. Wang,&al. (2005). *Effects of factor ix or factor xi deficiency on ferric chloride-induced carotid artery occlusion in mice*. J Thromb Haemost
49. Kilarski,&al. (2014). *Optimization and regeneration kinetics of lymphatic-specific photodynamic therapy in the mouse dermis*. Angiogenesis
50. Inai,&al. (2004). *Inhibition of vascular endothelial growth factor (VEGF) signaling in cancer causes loss of endothelial fenestrations, regression of tumor vessels, and appearance of basement membrane ghosts*. Am J Pathol
51. van Meeteren,&al. (2012). *Regulation of endothelial cell plasticity by tgf-beta*. Cell Tissue Res
52. Guc,&al. (2014). *Long-term intravital immunofluorescence imaging of tissue matrix components with epifluorescence and two-photon microscopy*. J Vis Exp
53. Randolph,&al. (2005). *Dendritic-cell trafficking to lymph nodes through lymphatic vessels*. Nat Rev Immunol
54. Drinker,&al. (1933). *Relation of the lymphatics to edema and the consequences of lymphatic obstruction*. Lymphatics, lymph and tissue fluid. The Williams & Wilkins Co.
55. Benichou,&al. (2011). *Immune recognition and rejection of allogeneic skin grafts*. Immunotherapy
56. Lund,&al. (2016). *Lymphatic vessels, inflammation, and immunity in skin cancer*. Cancer Discov
57. Lakkis,&al. (2000). *Immunologic 'ignorance' of vascularized organ transplants in the absence of secondary lymphoid tissue*. Nat Med
58. Yamagami,&al. (2001). *The critical role of lymph nodes in corneal alloimmunization and graft rejection*. Invest Ophthalmol Vis Sci
59. Fulmer,&al. (1963). *Transplantation of cardiac tissue into the mouse ear*. Am J Anat
60. McFarland,&al. (2009). *Skin allograft rejection*. Curr Protoc Immunol
61. Ruddle (2014). *Lymphatic vessels and tertiary lymphoid organs*. J Clin Invest
62. Gorecki,&al. (1991). *Evidence that liposome incorporation of cyclosporine reduces its toxicity and potentiates its ability to prolong survival of cardiac allografts in mice*. Transplantation
63. Colvin,&al. (2005). *Antibody-mediated organ-allograft rejection*. Nat Rev Immunol
64. Menkin (1931). *Studies on inflammation : Vii. Fixation of bacteria and of particulate matter at the site of inflammation*. J Exp Med
65. Menkin (1931). *Studies on inflammation : Vi. Fixation of trypan blue in inflamed areas of frogs*. J Exp Med
66. Menkin (1931). *Studies on inflammation : V. The mechanism of fixation by the inflammatory reaction*. J Exp Med
67. Menkin (1931). *Inflammation - a protective mechanism*. Arch circumscribe Med
68. Medawar (1948). *Immunity to homologous grafted skin; the fate of skin homografts transplanted to the brain, to subcutaneous tissue, and to the anterior chamber of the eye*. Br J Exp Pathol
69. Simpson (2006). *A historical perspective on immunological privilege*. Immunol Rev
70. Aspelund,&al. (2015). *A dural lymphatic vascular system that drains brain interstitial fluid and macromolecules*. J Exp Med
71. Barker,&al. (1968). *The role of afferent lymphatics in the rejection of skin homografts*. J Exp Med
72. Lambert,&al. (1965). *The role of the lymph trunks in the response to allogeneic skin transplants*. Transplantation
73. Joffre,&al. (2008). *Prevention of acute and chronic allograft rejection with cd4+cd25+foxp3+ regulatory t lymphocytes*. Nat Med
74. Lorentz,&al. (2011). *Engineered aprotinin for improved stability of fibrin biomaterials*. Biomaterials
75. Ferri (2014). *Ferri's clinical advisor 2013: 5 books in 1*. Elsevier Health Sciences.
76. Rutkowski,&al. (2006). *Characterization of lymphangiogenesis in a model of adult skin regeneration*. Am J Physiol Heart Circ Physiol
77. Rutkowski,&al. (2006). *Secondary lymphedema in the mouse tail: Lymphatic hyperplasia, VEGF-C upregulation, and the protective role of MMP-9*. Microvasc Res
78. Chakraborty,&al. (2013). *Lymphatic filariasis: Perspectives on lymphatic remodeling and contractile dysfunction in filarial disease pathogenesis*. Microcirculation
79. Patel,&al. (2015). *Lymphatic mapping and lymphedema surgery in the breast cancer patient*. Gland Surg
80. Olszewski,&al. (2015). *A novel method of edema fluid drainage in obstructive lymphedema of limbs by implantation of hydrophobic silicone tubes*. J Vasc Surg Venous Lymphat Disord
81. Palumbo,&al. (2002). *Spontaneous hematogenous and lymphatic metastasis, but not primary tumor growth or angiogenesis, is diminished in fibrinogen-deficient mice*. Cancer Res
82. Tammela,&al. (2011). *Photodynamic ablation of lymphatic vessels and intralymphatic cancer cells prevents metastasis*. Sci Transl Med
83. Pepper,&al. (2015). *A prevascularized subcutaneous device-less site for islet and cellular transplantation*. Nat Biotechnol

Supplementory figures

Supplementary Fig 1A. Lymph clots are forming within lymphatic collectors in peripheral lymphatics of B16/F10 tumor implanted under the ear skin.
Three weeks after implantation of tumor melanoma cells tumor mass formed palpable solid mass under the dorsal dermis of a mouse ear. The mouse was i.v. injected with FITC-labelled fibrinogen and six hours later blood circulation was flushed with Ringer's solution to remove blood from functional vessels. After that, the circulation was fixed with zinc-fixative, and the whole skin and tumor tissue were stained for basement membrane marker perlecan. Lymphatic collector vessels were identified by the presence of characteristic valves along which vessels change their diameter, from the narrow at the afferent tubular to wide at the efferent sinusoidal sides. Peritumoral lymphatic collectors had incomplete basement membrane and were also filled by autofluorescent erythrocytes that were also present outside vessels in the tumor interstitium (top two rows). However, in contrast to non-perfused (non-functional) blood vessels (bottom row), erythrocyte presence did not overlap with clotted labeled fibrin. Scale bar: 25μm.

Supplementary Fig. 1B

Supplementary Fig. 1B. Fibrosis in peripheral lymphatics of B16/F10 tumor implanted under the ear skin
A, B. Two examples of intralymphatic fibrosis identified at the edge of the lymphatic tumor. B16/F10 tumor cells were implanted for 7 days under the dorsal dermis of the ear. Arrows point to clusters of collagen I and collagen IV-positive matrix inclusions inside lymphatic collecting vessels. Arrowheads point to disorganized lymphatic endothelial cells with absent cell-cell junctions. The intensity of collagen IV was normalized to the signal level of weakest vascular structures present in the image. The intensity of collagen I was normalized to the average signal level of interstitial collagen. Scale bar: 50μm.

Supplementary Fig. 2 Comparison between active and partially active thrombin administration on intralymphatic and vascular blood clotting.

Confocal microscopy of whole-mount ear. A. Site of Intradermal injection: Injection of concentrated active thrombin (thrombin^{ac}) results in an instant but transient blood coagulation within blood vessels around the site of injection. Except for rare events, intralymphatic clotting was restricted only to the site around the injection area, and remote collectors were never occluded. Bl-blood vessels, L-lymphatics. B. Draining lymphatics: In contrast to active thrombin, two sequential injections of the mix of partially inactivated thrombin (1:6 active and inactive ratio, thrombin$^{in/ac}$) had no effect on blood vessel coagulation and induced intralymphatic clotting only in remote collectors with no effect on blood coagulation at the site of injection. Intralymphatic clotting was often associated with lymphatic leakiness around the clot location (interstitial fibrin deposits in the bottom, middle image). Scale bar: 50μm.

Supplementary Figure 3. Lymphatic regeneration by intralymphatic sprouting

Lymphatics regenerate by repopulation of ghost vessels. Eight days after photodynamic therapy (PDT), the state of lymphatic regeneration was observed by confocal microscopy on the whole mounted dermis. Ghost vessels, the remaining collector basement membrane sleeves stained with collagen IV), were filled with densely packed antigen presenting cells (CD45). Lymphatic endothelial cells (CD31, arrowheads) grow in close contact with the CD45+ cells. Scale bar: 50μm.

Supplementary Figure 4. Dendritic cells populate regenerating ´ghost vessels` after lymphatic-specific photodynamic therapy
A. Epidermal Langerhans cells, classic antigen presenting cells in the ear. In the epidermis, Langerhans cells create a dense, 2-dimensional and dendrite interconnected network that stains strongly for MHCII and CD11c. Basement membrane (BM) is stained with collagen IV. B. In the control region of the ear treated with photodynamic therapy (PDT), lymphatics are not populated with antigen presenting cells. C. In contrast, lymphatic collectors decellularized with PDT are densely populated with mostly double-positive MHCII+ and CD11c+ antigen presenting cells even 10 days after the treatment. Hf-hair follicles. Scale bar: 50μm.

Supplementary Figure 5. Lymphatic occlusion alone does not lead to persistent edema
Photodynamic therapy (PDT)-induced edema is transient and is resolved before lymphatic regenerate. 2 μg of Visudyne® (6x more than used to occlude the ear lymphatics) was injected in two sides of the tail with FITC-dextran. Draining lymphatics at a distance of 4 cm of the tail were irradiated with 25 J/cm2, and they were imaged with IVIS every day for 15 days. A. Example tail before edema development (day 0), during its peak (day 1 to 3 after PDT) and after the edema resolution (day 5, 7). B. Graph representing the edema development as measured by tail volume, and resolution after PDT.