Lightsheet Optical Tweezer (LOT) for Optical Manipulation of Microscopic Particles and Live Cells

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(Dated: July 6, 2021)

A light sheet based optical tweezer (LOT) is developed to trap microscopic dielectric particles and live HeLa cells. The technique requires generation of tightly-focussed diffraction-limited light sheet which is achieved by a combination of cylindrical lens and high NA objective lens. The field pattern generated at the geometrical focus is a tightly focussed line (along x-axis) perpendicular to the beam propagation direction (z-axis). Spherical beads undergoing Brownian motion in the solution were trapped by the gradient potential and the travel time is estimated from the fast CMOS camera (operating at $230 frames/sec$). High speed imaging of beads show the stiffness of LOT system to be $\sim 0.00118\ pN/nm$, which is an order less than that of traditional optical point-traps. The trapped beads displayed free movement along the light-sheet axis (x-axis) displaying one-degree of freedom. Subsequently, LOT technique is used to optically trap and pattern dielectric beads and HeLa cells in a line. We are able to successfully pattern 8 dielectric beads and 3 HeLa cells in a straight line. We anticipate that LOT can be used to study 1D-physics of microscopic particles and to understand patterned growth of live cells.

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Optical tweezers (OTs) are known to play key roles in understanding molecular forces (or torques) and mechanical properties of proteins (DNA, RNA etc.). In addition, this techniques has applications in optical sorting (sorting cells [2] [3], sorting colloidal spheres [1]), and single molecule biophysics [4] [5]. The delicate force exerted by radiation have consequences in precision measurement and low force applications (sub-piconewton).

In the year 1970, Arthur Askhin was the first to show that micron-sized latex spheres suspended in water can be manipulated [6]. Subsequently, the first demonstration of single beam optical tweezers was carried out and successful trapping of bacteria and red blood cells were carried out [7] [8]. The basic physics of optical tweezers revolves around the fact that light carry linear and angular momentum, and this can be harvested to manipulate microscopic particles both inside and outside live cells. The forces that compete and need to be balanced for a stable trap are gradient and scattering forces. For his pioneering work on optical tweezers, A. Askhin received nobel prize in the 2018 [9]. The field is growing at a rapid pace and finding new application across the disciplines of science and engineering.

Light focused by spherical optics (such as biconvex lens and objectives) produces point focus with maximum intensity at the centre. This gives rise to a well-defined point traps when focussed by light with a Gaussian beam profile (such as laser). Both sub-micron and micron sized particle can be trapped and manipulated using point traps. This is different for cylindrical lens system that focus light to a line rather than point. As a result, the particle trapped in a focal-line has one-degree of freedom but restricted in the other two directions. Historically, light sheet was first generated by Siedentopf and Zsigmondy in 1903 to observe gold particles [10]. Later on, a modernized version of light sheet microscopy was built using cylindrical lens in 1993 by Voie et al. [11]. Subsequently, light sheet was diversified by Stelzer and Keller for biological imaging [12] [13] [14]. The technique has seen applications in diverse fields ranging from biological sciences (biological imaging [15] [16] [17] [18] [19] [20], iLIFE imaging cytometry [38] [21]) to physical sciences (nanolithography [24] [25], optics [22] [23]). The last decade has seen an emergence of several important variants of light-sheet systems. Some of these include thin light-sheet microscopy [26], ultramicroscopy [27], objective coupled planar illumination microscopy (OCPI) [28], confocal light-sheet microscopy [29][30], multiple light-sheet microscopy [31], dual-inverted selective-plane illumination microscopy (diSPIM), [32], light-sheet theta microscopy (LSTM) [33], open-top light-sheet (OTLS) [34][35] and lattice light sheet microscopy [36], LVLSM [37] and IML-SPIM [17]. These variants offer many useful configuration for generating light sheets that can be used for demanding applications.

In this letter, we propose and develop lightsheet optical tweezers (LOT) for trapping microscopic objects. This is accomplished by generating diffraction-limited light sheet using a combination of cylindrical lens and high NA objective lens. A stable and confined optical trap is produced and the same is used to demonstrate trapping of dielectric beads and live HeLa cells.

The theory of line-traps (generated by light sheet) is similar to that of point focus with the exception that particle has complete freedom along one dimension. Unlike point-traps that are better understood in the cylindrical coordinate system (r, z, with r being the lateral/radial plane and z being the beam propagation direction), LOT is better understood in Cartesian coordinate system (x, y, z) as shown in Fig. 1. The diffraction-limited light sheet is taken along xz-plane with x along the lightsheet axis and z along the propagation direction. From Fig. 1, the cylindrical lens focus light to a line extending along y-axis. The objective lens is placed at the focus of cylindrical lens. The field focussed at the back-aperture of objective lens undergoes Fourier transform, forming a diffraction-limited vertical line at its focus. In general, two cases arise: (1) the particle is much smaller than the wavelength of light (Rayleigh regime), and (2) the particle is larger than the wavelength of light (Geometric regime). We briefly discuss both the cases.

In the Rayleigh regime, we consider a dielectric particle in a laser beam and that the size of particle is much smaller than wavelength of light. In this regime, the particle behaves as a Rayleigh scatterer, and its reaction to the light field $\vec{E}(x,y,t) = re\{\vec{E}_0(x,y)\ e^{i\omega t}\}$ is determined by its polarizability (α). The electric field on the particle induces a dipole moment, $\vec{\mu}(x,y,t) = \alpha\ \vec{E}(x,y)$, and the energy of induced dipole is, $U = -\vec{\mu}(x,y,t).\vec{E}(x,y) = -\alpha I(x,y,t)$, where, $I(x,y,t) = |E_0^2|$. This immediately states that the energy of dipole assumes minimum at a position where the intensity is maximum, resulting in a well-defined trap location (i.e, x, y). This rules out optical trapping for a uniformly intense light source, and thus a non-uniform intensity profile such as those for Gaussian beam is desired. In a lateral case of beam with Gaussian intensity profile, the dipole (particle) is expected to experience a force towards higher intensity i.e, the beam centre. The corresponding force along y is given by, $\vec{F}_y^g = \frac{\partial U}{\partial y} = -\alpha\frac{\partial}{\partial y}I(x,y,t) = -\alpha\frac{\partial}{\partial y}\langle\vec{E}(y,t)^2\rangle = -\frac{\alpha}{2}\frac{\partial}{\partial y}|E_0(y,t)|^2 = \beta\frac{\partial}{\partial y}I_0(y,t)$, where, $\langle ...\rangle$ is the time average, and $\langle\vec{E}(\vec{r},t)\rangle = |E_0|/2$. Note that, the variation of intensity is negligible and does not change appreciably along x except at the far ends.

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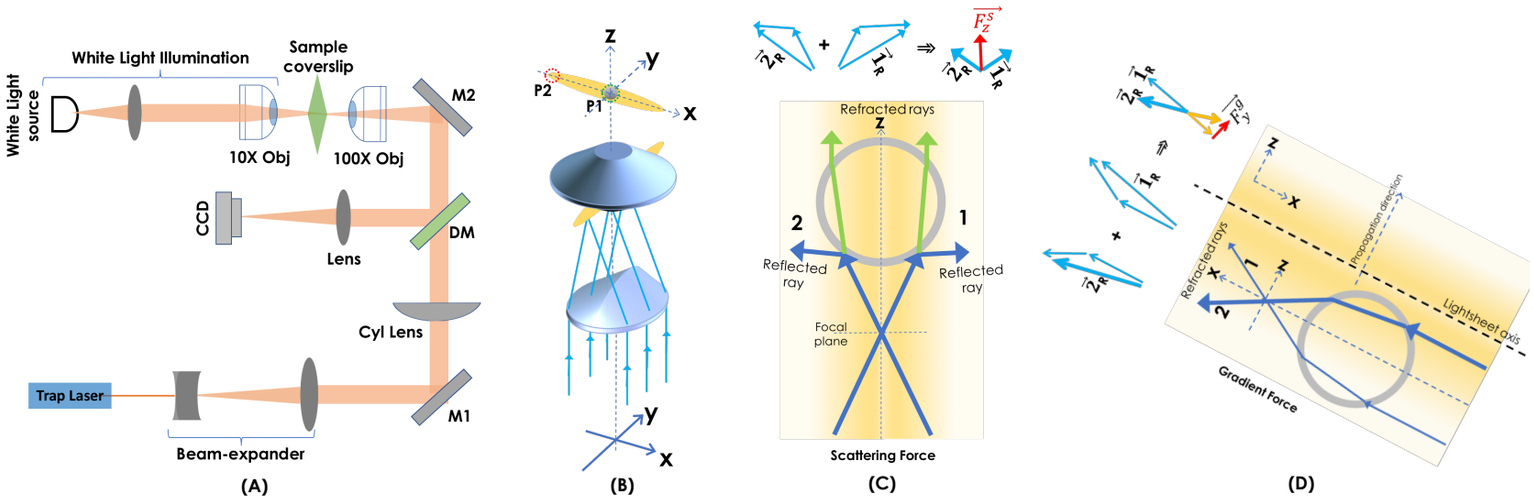

FIG. 1: (A) Schematic diagram of the developed lightsheet optical tweezer (LOT) system. (B) The combination of cylindrical lens and high NA objective lens for generating diffraction-limited light sheet. (C) The resultant scattering force (due to the reflection of light) acting on the micro-particle along z-axis. (D) The gradient force acting inwards (towards lightsheet axis) on the particle along z-axis.

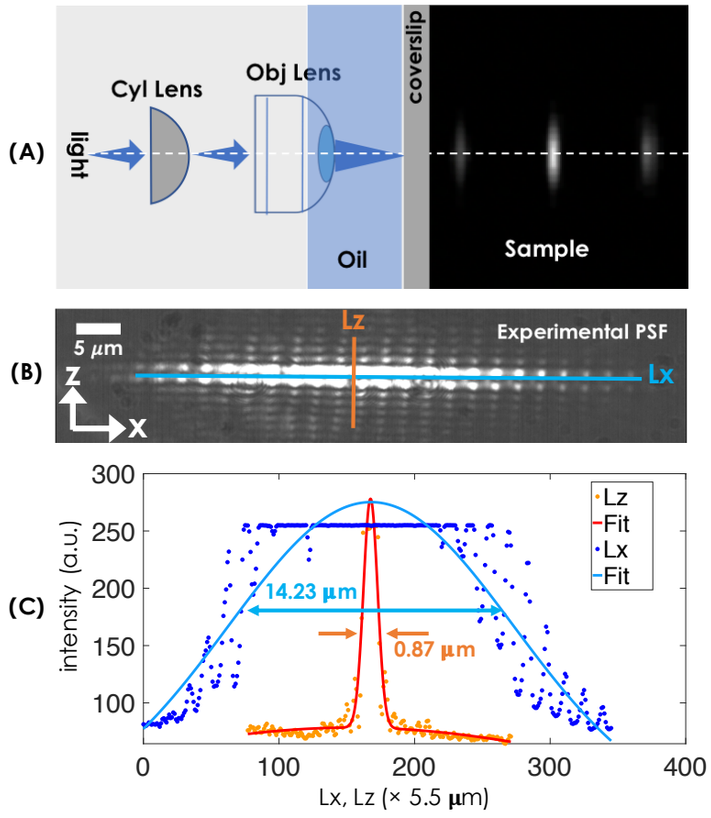

FIG. 2: (A) Schematic showing the formation of light sheet by a combination of cylindrical and oil-immersion objective lens in the specimen. (B) The reflected image of light sheet formed in the cell medium (DMEM) as observed by the camera. (C) Intensity plots across the light sheet (blue and orange line) and the and the Gaussian fit function show the actual size of light sheet to be, $0.87\ \mu m\ \times\ 14.24 \mu m\ (z \times x)$.

Hence, $\vec{F}_x = \frac{\partial U}{\partial x} = \beta \frac{\partial}{\partial x} I_0(x,t) = 0$ along x is In the above expression. We have absorbed the refractive index and permittivity in a single parameter, $\beta = \alpha/2cn\epsilon_0$, where n is the refractive index of the particle and ϵ_0 is the permittivity of vacuum. Accordingly, the particle is trapped when the polarizability of particle is greater than the surrounding media. In the geometric regime, where the particle size is larger than the wavelength of light such as dielectric beads, ray-optics can be employed to understand force acting on the bead / particle. Classically, force on the particle can be defined as the rate of change of momentum, $F = \frac{\partial \vec{p}}{\partial t}$, where $\vec{p}$ is the momentum of the particle. The refracted light results in a change of momentum (change of ray direction) with larger momentum at higher intensity (see, Fig.1D), this generates a recoil force F_{refac} (see, red arrow) for off-focal bead, ultimately pulling the particle towards centre of line-focus (lightsheet axis). A similar force but in opposite direction appears when the particle is on the other side of light sheet axis. The recoil forces along y and z direction are essentially the gradient forces $\vec{F}_y^g$ and $\vec{F}_y^g$, respectively.

Now, let us determine the role of scattering force F_s. Primarily, the scattering occurs due to reflection of light, and the scattering force in Rayleigh regime can be expressed as, $\vec{F}_s = \frac{n_m\ \sigma_s}{c} \langle \vec{S}_i \rangle$, where, σ_s is the cross-section of particle. Fig.1C shows the resultant scattering force ($\vec{F}_s^z$) due to the reflection of light at the bead surface. This occurs in the direction of Poynting vector $\vec{S}_i$ which is also the direction of beam propagation and has a unit of energy per unit area per unit time. So, scattering force has the direction of Poynting vector i.e, it tends to push the particle out of focus along the light propagation. Accordingly scattering (i.e, reflected light at the back of bead) tend to push the particle out of focus with a force F_{reflec} (which is also known as the scattering force, $\vec{F}_z^s$). Now since the momentum is conserved, and there is a transfer of momentum between the particle and light, it is possible to balance these forces to obtain a stable trap (see, Fig.1D). So, gradient intensity with maximum intensity at the centre lead to stable trap both along y-axis, and along the beam direction (z-axis). In LOT, the bead is free to move along x-axis due to lack of intensity gradient. Overall, the condition for three-dimensional stable trap is achieved when the gradient potential overcomes the other forces (radiation pressure / scattering force, buoyant force, and the forces due to Brownian motion and gravity).

The next logical step in the development of LOT is to determine the trap-stiffness. We used spherical transparent beads as as the sample to determine trap-stiffness. Within the influence of gradient force, the particles/beads undergoing Brownian motion are attracted to the trap centre. To a good approximation, an optical trap behaves like a harmonic potential, and it is able to exert a restoring force. Specifically, near the trap centre, the force can be approximately

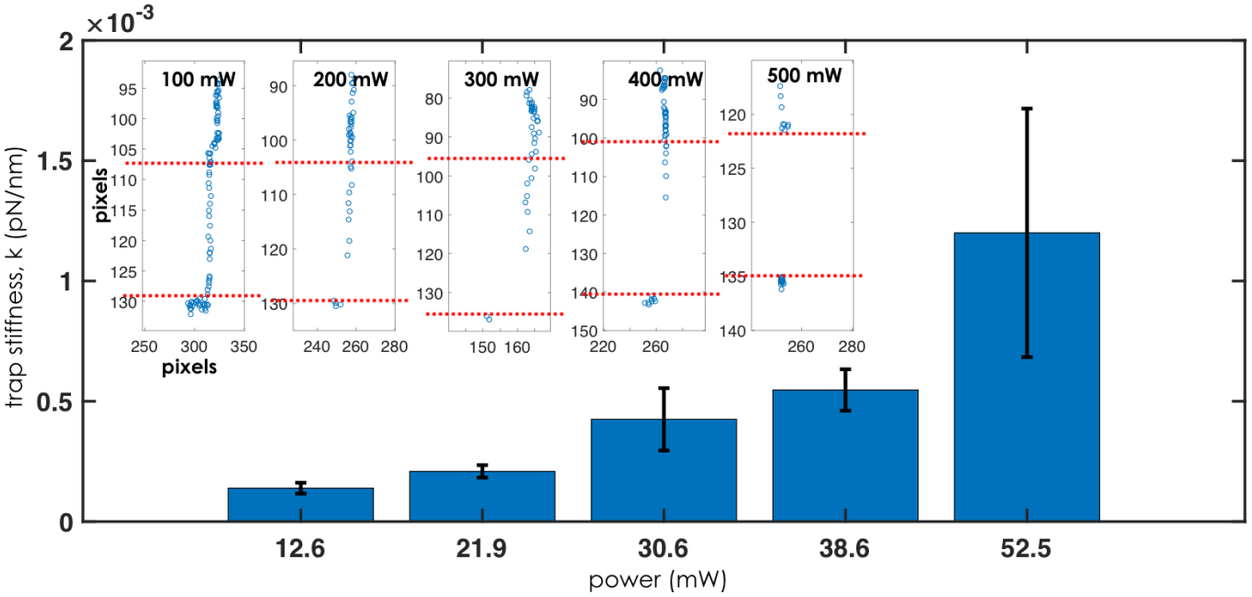

FIG. 3: Trap stiffness k (pN/nm) of LOT at varying light intensity, $12.6 - 52.5$ mW. The insets show time taken by a single bead to reach trap-centre with increasing intensity, where the number of blue dots indicate the number of frames taken during the trapping process.

modelled by Hooke's law and the restoring / gradient force is given by, $V(x) = -kx$, where k is the trap stiffness (N/m) and x is the travel distance / displacement from the trap origin. The second force acting on the particle is viscous drag force. Assuming spherical particle (beads), the particle moving through the fluid experiences a viscous force of, $F_{vis} = -6\pi\eta r_b v$. For simplicity and calculating approximate trap-stiffness, we neglect the effect of gravity on the bead so forces due to weight and buoyancy can be ignored. The motion of bead is governed by these two forces (gradient and viscous/drag force) which are opposite to each other. Balancing optical (gradient) forces with drag force produces [39] [40], $-kx = -6\pi\eta r_b v \Rightarrow k = 6\pi\eta r_d(v/x) \quad \Rightarrow k = 6\pi\eta r_d/t$, where $x = vt$ and, v is the dragging velocity, x is the displacement and t is the time, η is the medium viscosity, and $r_d = d/2$ is the bead radius.

The schematic diagram of the developed optical tweezer (LOT) is shown in Fig. 1A. The picture of actual optical tweezer is shown in the **Supplementary Fig. S1**, and related description can be found in **Supplementary material**. A trap laser light of wavelength 1040 nm is used to trap dielectric silica beads (Thorlabs, USA). The laser beam is expanded 5 times by the beam expander so as to fill the back-aperture of cylindrical lens (Cyl Lens, $f = 150$ mm). The lens focusses light along y-axis on to the back-aperture of 100X objective lens (Olympus, 100X, 1.3 NA), without any change along x-axis. The line focus at the back-aperture of objective lens gives rise to an orthogonal diffraction-limited line-focus (see, Fig. 1B). A separate illumination sub-system is integrated for visualizing the specimen (beads suspended in distilled water). This consists of a white light source a condenser lens and a low NA objective lens (Olympus, 10X 0.3 NA). The lens illuminates a larger field-of-view (FOV) of the sample plane, and the transmitted light is collected by the 100X objective lens (Olympus, 100X 1.3NA). The light then pass through the dichroic mirror (DM) to the tube lens which focus it to the fast CMOS camera (Gazelle, Pointgray, USA). A schematic of the key optical element for generating light sheet trap is shown in Fig. 1B. Note that, the light sheet generated by the cylindrical lens is projected on to the back-aperture of high NA objective lens that give rise to an diffraction-limited light sheet at the focus. The line focus is formed along the x-axis and orthogonal to propagating direction (along z-axis). The resultant field and trap geometry is shown in Fig. 2. Two major forces (gradient force and scattering force) acting on a spherical bead are shown in Fig. 3(C,D). The scattering force on the particle is towards the beam-propagation direction (z-axis outwards) that pushes the particle away from the light sheet centre (see, red arrow for $\vec{F}_z^s$). The corresponding vector forces acting on the particle is shown in Fig. 1C. On the other hand, the gradient force is primarily due to refraction and exerts a restoring force on the particle when it is away from the centre (lightsheet axis). So, the gradient force pushes the particle towards high intensity which is the centre of trap (see, red arrow for $\vec{F}_z^g$). This is explained based on the vector force diagram shown in Fig. 1D. Unlike point-traps where particle experience gradient forces radially inwards (along $\vec{r} = \sqrt{x^2+y^2}\ \hat{r}$. LOT involves particle trapping along y-direction only. This leaves the particle free to move along x-axis without experiencing any net force.

Trapping micro-particles require a strong, stable and confined optical field (system PSF). This can be generated by focussing high intensity light by a high NA objective lens. The schematic diagram of the key optical component along with the formation of light sheet is shown in Fig. 2A. The field is shown at discrete values of z in the specimen. Fig. 2B shows the actual field recorded by the camera (in the reflected mode) for a combination of cylindrical lens ($f = 150$ mm) and high NA objective lens ($100X$, 1.3 NA). Visually, the field displays optical aberration in the specimen medium predominantly due to multiple reflections and medium inhomogeneity. Alongside the intensity plots are also displayed (see, Fig. 2C). Gaussian function is fit to the data to determine the dimension of light sheet. The size of light sheet is estimated as 14.23 μm along x-axis and has a thickness of 0.87 μm.

Experimentally, the travel time (t) can be calculated from the number of frames (of the recorded video) from the initial position (particle undergoing Brownian motion) to final position (trap-centre) using a high-speed camera (CMOS camera). From the video, several beads are tracked on their way to the trap-centre, and the time is computed (from top to bottom dotted red line in Fig. 3). It is clear that beads take more time / frames (represented by blue dots) to reach trap-centre at low light when compared to intense light (see inset in Fig. 3). This is understandable since low power produce weak optical trap. Other important parameters include mass ($m = \rho V$) of the bead can be calculated from the density of bead ~ 2000 Kg/m^3, and its volume (assuming spherical shape, $V = (4/3)\pi(d/2)^3$, where d is the diameter). The average time between two consecutive position of the bead or $\#frames$ (represented by blue dot in the track-plot) is chosen

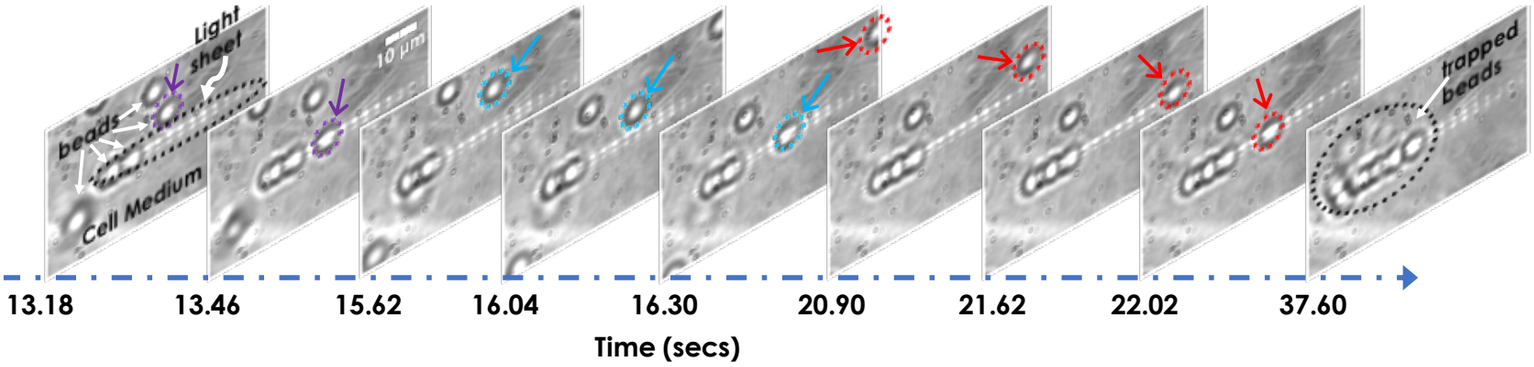

FIG. 4: Images taken during sequential trapping of several beads to pattern beads in the form of a chain. All the beads displayed undergoing Brownian motion. Few beads in close proximity to the light sheet are indicated by violet, blue and red circle/arrow that are eventually trapped in the process. The respective timeline is shown below. The entire process is encapsulated in the **Supplementary Video 1**.

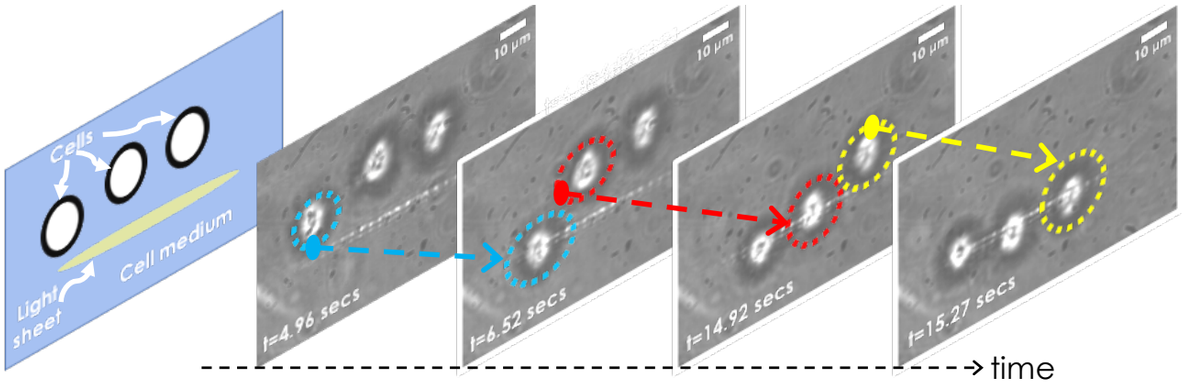

FIG. 5: LOT technique is used to trap HeLa cells suspended in cell medium (DMEM). The cells were trapped and manipulation one-by-one and aligning in a line. See **Supplementary Video 2**.

as, 9.4 *msec* (camera frame-rate). Knowing that, the viscosity of water at 25^oC is, $\eta = 0.8925 \times 10^{-3}\ Pa.\ s$, the average trap stiffness of LOT can be calculated using, $k = 6\pi\eta r_b v/t = 16.82 \times 10^{-9}/t\ pN/nm$. A better estimate can be arrived at by taking into account other forces. Fig. 3 shows the trap stiffness (k) at varying light intensity. It is immediately evident that, light sheet traps are an order weaker than typical point traps. This is predominantly due to the fact that light sheet PSF is spread over a larger space (along a line) than a point, and so the intensity is much weaker than that of a typical point-trap.

To visualize the functioning of LOT system, we used dielectric beads suspended in distilled water as a sample. A drop of specimen is dropped on the glass-covership and then it is placed on the oil-dipped 100X objective lens. The light sheet is generated in the water medium as shown in Fig. 4. The beads can be seen randomly distributed with one of the beads on the light sheet. Schematic of the trap experiment is shown in Fig. 4. At time $t = 13.18$ *secs*, two beads are trapped and one bead (marked by violet arrow and circle) is bear the light sheet. In the frame (recorded at 13.46 *secs*), the bead is trapped by the gradient potential. The next frame (taken at $t = 15.62$ *secs*) shows an approaching random bead (marked by blue arrow) which is seen attracted by the potential in the subsequent two frames. The same can be observed for the next bead (marked by red arrow). Over time a number of beads are arranged on a line (light sheet) as seen from the image taken at 37.60 *sec*. The entire process can be seen in the **Supplementary Video 1**.

Cell-cell interaction (interaction between cell surfaces) play crucial role during early development of multicellular organisms. These interactions allow cells to communicate with each other in the microenvironment (culture medium). It is the communication between the cells that controls its growth at a healthy rate. Uncontrolled growth are known to occur in cancer. Here, we use LOT to arrange cells in a line and study their growth for the next 24 hours. Fig. 6A shows HeLa cancer cells grown on a coverslip. These cells are attached to the coverslip surface and can be seen randomly-oriented. To detach from the surface, the cells were trpsinated (using ... of Tripsine solution) for 4 minutes. This is followed by centrifuging and resuspending the cells using the cell medium (DMEM). Subsequently the floating cells were subjected to light sheet trap. One-by-one the cells were trapped by the light sheet field and aligned in a line as displayed in Fig. 6. The corresponding time line is also shown. The entire process can be visualized in **Supplementary Video 2**. This shows that the technique is capable of patterning cell in a preferential direction that can help understand cell-cell interaction both at a single cell level and in an ensemble.

We propose and demonstrate the first lightsheet tweezer for trapping dielectric particles. Unlike traditional point-trap tweezers, LOT can trap particles in a line and the particle has single degree of freedom along the light sheet axis. LOT is used to demonstrate trapping of dielectric beads suspended in distilled water. From the time-travel of particle to the epicentre of trap, the stiffness of 1D potential is determined by calculating time using a high speed CMOS camera. We showed a maximum trapping of 8 beads and 3 HeLa cells in a light sheet. LOT are highly scalable and can be used to trap few to several particles. Further progress of LOT may lead to 2D planar traps, and the light sheet can be modified to realize this, possibly using a low NA objective and a high laser power. This technique may find application in colloidal physics, particle patterning, and patterned cell growth in cell biophysics.

Acknowledgements: The authors acknowledge financial support from parent institute (Indian Institute of Science, Bangalore, India). PPM conceived the idea. AS, JB, PJ, NB, PPM carried out the experiment. AS, PJ, NB prepared the sample. PPM wrote the paper by taking inputs from all the authors.

Data Availability: The data that support the findings of this study (including the 3D volume of the specimens) are available from the corresponding author upon request.

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