Bounded rational decision-making models suggest capacity-limited concurrent motor planning in human posterior parietal and frontal cortex

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Abstract

While traditional theories of sensorimotor processing have often assumed a serial decision-making pipeline, more recent approaches have suggested that multiple actions may be planned concurrently and vie for execution. Evidence for the latter almost exclusively stems from electrophysiological studies in monkeys. We here study concurrent prospective motor planning in humans by recording functional magnetic resonance imaging (fMRI) during a delayed response task engaging movement sequences towards multiple potential targets. We find that delay activity in posterior parietal cortex, frontal cortex and the cerebellum modulates both with sequence complexity and the number of potential targets. We tested the hypothesis that this modulation is best explained by concurrent prospective planning as opposed to the mere maintenance of potential targets in memory. We devise a bounded rationality model with information constraints that optimally assigns information resources for planning and memory for this task and determine predicted information profiles according to the two hypotheses. When regressing delay activity on these model predictions, we find that the concurrent prospective planning strategy provides a significantly better explanation of the fMRI-signal modulations. Moreover, we find that concurrent prospective planning is more costly and thus limited for most subjects, as expressed by the best fitting information capacities. We conclude that bounded rational decision-making models allow relating both behavior and neural representations to utilitarian task descriptions based on bounded optimal information-processing assumptions.

keywords: information capacity, human motor planning, fMRI, prospective planning, bounded rationality model, SPL, PRR, IPS, PMd, DLPFC, cerebellum

1   Introduction

Traditional theories of sensorimotor processing often consider a sequential pipeline from perception to action, where in between the cognitive system makes a decision that is subsequently implemented by the motor system that plans and executes the corresponding action [1, 2, 3, 4, 5, 6]. In this view perceptual, cognitive, and motor representations

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do not overlap and are separated in time. Thus, it is often assumed that the value of different alternatives is computed and used for decision-making in prefrontal regions, which is then subsequently translated into action planning in premotor regions, including parietal, precentral, and subcortical regions [1]. In contrast, more recent frameworks, like the affordance competition hypothesis [7, 8], have put forward the notion that actions might be planned concurrently in several frontoparietal brain areas and vie for execution, whenever opportunities for multiple potential actions arise at any one time.

Neurophysiological studies in monkeys have found increasing evidence, that multiple potential actions are planned in parallel and competitive potential plans are simultaneously represented in posterior parietal cortex (PPC) [9] and dorsal premotor cortex (PMd) [10, 8]. Moreover, it has been suggested that neurons that are involved in motor planning are often also involved in the decision-making process [11, 8]. In how far particular decisions are accompanied by more integrated or more serial processing may also depend on the task specification, as shown by Cui et al. [2] for spatial and non-spatial decisions. In particular, their results show that different areas in the posterior parietal cortex encode both potential and selected reach plans (parietal reach region) or encode only selected reach plans (dorsal area 5), suggesting a parallel visuomotor cortical circuitry for spatial effector decisions. Some studies have even suggested that concurrent planning can take place after movement onset in a way that is effecting movement kinematics and variability during reaching [12, 13, 14].

While there is also evidence for neural correlates of prospective planning in humans in posterior parietal and premotor cortex such as in superior parietal lobule (SPL), anterior intraparietal sulcus (antIPS) and PMd [15], so far most evidence for *parallel* prospective planning has been acquired in monkey studies. Here we ask whether 1) concurrent prospective action planning also happens in humans and 2) if there is an individual capacity limit for concurrent planning and how this could be quantified.

Similar to previous studies that have quantified the capacity of working memory using information theory to measure how well different items can be told apart [16, 17, 18, 19, 20, 21, 22, 23, 24], we use information theory in the following to quantify processing capacity also in the context of sensorimotor tasks. This can be achieved by designing optimal choice models with information constraints resulting in an abstract model of bounded rational decision-making where resources are measured in units of information [25], with the understanding that ultimately any other resource measure (like time or energy consumption) can be converted into limits on processed information. A bounded optimal decision maker trades off these informational costs he needs to invest to form an action policy against the expected utility of this policy. For a goal-reaching we assume a utility function that assigns a reward to those actions that will hit a target.

In previous studies [26, 27], we have investigated such optimality models with information bounds in the context of motor planning by manipulating both permissible reaction times and prior distributions over possible world states. In these behavioural experiments reaction time was used as a proxy for information cost underlying any process of uncertainty reduction. Here we applied such bounded rational decision-making models to human fMRI activity in order to reveal whether brain areas engaged in the planning of goal-directed actions resort to a delayed planning strategy or, alternatively, to concurrent prospective planning. In addition we used these models to estimate planning-related capacity limits. We show that brain activity in a parietal-frontal planning system and the cerebellum is consistent with a bounded optimal information flow implementing concurrent prospective action planning.

Figure 1: (A) The four target planning conditions differed in the number of potential target locations initially cued. Subjects could see possible target positions highlighted (grey boxes). Potential targets to consider for planning were indicated by a grey frame around the field areas encompassing the relevant possible targets. Subjects were instructed to plan a single movement sequence towards one target ('1'), two partially overlapping sequences towards two potential targets ('11'), two distinct movement sequences towards two potential targets in different panels ('2'), or four distinct movement sequences towards four potential targets ('4') respectively and to execute the planned movement in the following phase, after the ultimate target was revealed by the go-signal. (B) Trials of the motor planning conditions in the delayed response task (DRT) and control condition (CT) were randomized and had a similar timeline. Each trial started with a fixation period (FIX) of random duration, a cue phase (CUE) followed by a random dot pattern to mask afterimages of the CUE (MASK), a delay phase (DEL) of random duration for planning, and a response phase (RES). In the response phase the ultimate target location was revealed by a go-signal, namely a single grey frame around the relevant (part of the) respective response panel. In the control task, no potential target cues were presented during the cue phase and therefore no goal-directed actions could be planned during the delay phase. In the response phase of the CT subjects were finally informed about the target location (single grey box).

Figure 2: Information theoretic model hypothesis of bounded optimal planning with information constraints. (A) Information about the hidden world state $w \in \mathcal{W}$ (the exact target location) is revealed in two steps during the experimental trial. The initial cue stimulus $s_1 \in \mathcal{S}_1$ indicates all potential target locations while the later go-signal s_2 resolves any remaining uncertainty about the actual hidden target w. (B) When seeing s_1, the decision-maker can in a first step form a memory $m \in \mathcal{M}$ which is required to extrapolate on the world state when seeing s_2 after the delay and, therefore, is then able to appropriately plan and finally select an action $a \in \mathcal{A}$ that corresponds to a movement path representation. Both hypothesis (H0 and H1) contrast the predicted information I_1 and I_2 in all 12 DRT conditions for a delayed planning strategy and concurrent prospective planning strategy during the delay (DEL). H0: During the delay phase only memory m is used to reduce uncertainty about actions. H1: Concurrent prospective planning of actions during delay phase requires the anticipation of all possible selection stimuli s_2 and planning movement sequences in parallel. I_2 therefore is higher in H1 than in H0 and, moreover, varies more strongly with movement sequence length. (C) Model Comparison. We correlated theoretical memory and prospective planning information with measured fMRI activity in relevant brain areas during the delay phase and tested two hypothesis: H0, where information costs correspond to uncertainty reduction only based on memory m and H1, where higher information cost for prospective planning is required to anticipate possible future events. Theoretical information I_1 and I_2 of the bounded rationality model for different memory and planning capacities, defined by model parameters β_1 and β_2, were regressed (using regression coefficients α_1 and α_2) with the measured fMRI BOLD activity. For lower β_1 and β_2, memory and planning capacity accordingly is more limited. We regressed the information values for different degrees of boundedness and compared the best model fits with the predicted information in the not-bounded case, where β_1 and β_2 were chosen high ($\beta_1 = 500$, $\beta_2 = 500$).

2   Results

The experimental paradigm of the present study was designed to contrast a serial memory-based planning strategy ("delayed planning") and a parallel prospective planning strategy ("concurrent prospective planning") to prepare for a goal-directed action in a delayed-response scenario (compare Figure 1). To this end we used a delayed response task (DRT), in which an *initial "cue"* revealed multiple potential target locations. During a subsequent delay period, subjects were instructed to prepare for the upcoming response. The ultimate target location was, however, only revealed after the delay, namely through an additional *"go-signal"* presented in the response phase. Note that our delayed response paradigm thereby allowed us to temporally isolate brain activity related to the planning of actions both from the sensory responses elicited by the visual cues (initial cue and go-signal) and from activity related to motor execution [15]. Moreover, our task allowed us to distinguish whether planning activity during the delay can be attributed to delayed planning or, alternatively, to concurrent prospective planning, namely by considering the task-specific information costs associated with each of the two respective strategies, as will be detailed in the following.

In our delayed-response task information about the hidden world state $w \in \mathcal{W}$ (the ultimate target location) is revealed by the two stimuli, that are presented successively: the initial cue stimulus $s_1 \in \mathcal{S}_1$ indicates all potential target locations; the second go-stimulus s_2 resolves the remaining uncertainty about the actual hidden target w (see Figure 2 A). In principle, either serial or parallel processing could be chosen to appropriately prepare an action policy during the delay phase (see Figure 2 B), from which an action $a \in \mathcal{A}$, which corresponds to a movement sequence, can be finally be selected during the response phase. In either case, the overall process can be described with two information quantities (I_1 and I_2), that are dependent on the respective task condition (e.g. the number of potential targets and/or the length of the action sequence that leads to these targets). In a first step, an information cost I_1 is needed to form and maintain a memory of the initial cue $m \in \mathcal{M}$, which is required for the decision-maker to extrapolate on the world state when seeing s_2 after the delay. The process of memory formation therefore resolves some uncertainty about w in the extent of the information that s_1 provides. This process and its associated information cost I_1 is identical in both planning strategies, delayed planning and concurrent prospective planning. In a second processing step, uncertainty about actions gets reduced. This requires an additional information cost I_2, that, however, differs for the delayed planning and the concurrent prospective planning strategy. In the delayed planning scenario, only memory m is used to reduce uncertainty about actions and further information processing suspended until the go-stimulus s_2 gives further information and indicates the hidden world state. For concurrent prospective planning, however, all potential target locations are considered and information costs add up for all respective action sequences towards these targets. I_2 therefore is generally much higher but is also increasing more strongly with movement sequence length for a concurrent prospective planning strategy as compared to a delayed planning strategy (see Figure 2 C). This difference in integrated information costs I_1 and I_2 would allow us to probe whether fMRI activity in the delay period does reflect concurrent prospective planning (hypothesis H1) or serial delayed planning (hypothesis H0). Moreover, while prospective parallel planning brings essential benefits by enabling subjects to react more quickly to an upcoming scenario [28], it is immediately clear that this type of parallel planning cannot be applied indefinitely and that there must be bounds on the amount of information processing. For this reason we also assess these capacity limits of information processing.

Behavioral performance analysis

In our delayed-response-task (DRT), 19 subjects (11 females, 8 males, average age $=$ $= 27.5$) were shown an initial cue stimulus with potential target locations that were highlighted in four concentrically ordered response panels. They were verbally encouraged during the subsequent delay phase to plan movement sequences to all potential targets, and to execute one of these sequences, when shown the go-signal as a selection stimulus during the response phase (see Figure 1 B). Movement sequences could vary in sequence length (2-step, 3-step and 4-step condition) and consisted of up/down/left/right button clicks to move a cursor on a screen. To enforce planning during the delay phase, the go-signal did not indicate the actual selected target directly, but only indicated the relevant (part of the) response panel. In other words, subjects could uniquely identify the selected target only if they remembered the information I_1 provided by the initial cue stimulus. In total, our task design contrasted 3x4 DRT conditions, that did not only vary both in the movement sequence length (2, 3, or 4), but also in the number of potential targets (1, 2 or 4 targets in distinct response panels or condition '11' with 2 targets in the same panel). Consequently, the 12 DRT conditions were distinguished by different information costs due to multiplicity of potential panels, potential targets and sequence lengths.

We assessed subjects' behavioral performance in terms of reaction times, movement times and error rates and compared to a control condition (CT), where the initial cue stimulus did not contain any information about the target location but the relevant target location was explicitly cued during the response phase. Therefore subjects did not need to memorize or plan during the delay.

We found that reaction times increased with the number of potential targets ($p < 0.0001$, 2-way rmANOVA with factors condition ['1','11','2','4','CT'] and sequence length: linear effect of condition – see Methods section for details on the statistical analysis), suggesting that subjects engaged in more complex planning as the number of potential targets increased (Figure 3 A). In contrast, sequence length had no significant effect on reaction times ($p = 0.441$). The opposite pattern of results was revealed for movement time: there was a significant effect of sequence lengths on movement times as shown in Figure 3 B ($p < 0.0001$, 2-way rmANOVA with factors condition ['1','11','2','4','CT'] and sequence length: linear effect of sequence length). There was no linear effect of condition on movement time ($p = 0.449$).

Compared to the DRT conditions, the control condition CT did not allow for any planning during delay. In case of concurrent prospective planning (but not for delayed planning), we therefore expected to reveal reaction time benefits in DRT as compared to CT. Indeed, reaction times in the less costly planning conditions '1' and '11' were significantly reduced as compared to CT ($p < 0.0001$ and $p = 0.004$, respectively; 2-way rmANOVAs factor condition). For the two more complex planning conditions '2' and '4' no such a reaction time advantage was found (see 3 A).

In the CT, the target was explicitly shown after the delay, which perhaps explains the lowest error rates in this condition (see Figure 3 C). In contrast, the DRT conditions required memorization of the cue stimulus, which allowed for additional errors and thus led to higher error rates in the more complex DRT conditions ($p = 0.001$, rmANOVA, condition '4' vs. CT, $p = 0.002$, rmANOVA, sequence length 2 vs. 3). During the delay phase the number of saccades per second did not significantly differ between the different planning conditions and control conditions (see Figure3 D). This absence of difference in eye movements during the delay phase will be important in the next section, where we study fMRI activity during the planning delay period and need to exclude additional

effects on fMRI from eye movements.

fMRI analysis

Brain activity during task performance was measured by means of fMRI in a 3T MRI scanner. We fitted a general linear model (GLM) to the activity time series data measured in each subject and in each voxel of the brain. In this GLM we modeled each of our 4x3 conditions and separately for cue, delay and response phase (for details see methods). We used the resulting regression models to determine regions of interest that show significant functional delay-related activity on the group level. To this end, the delay-related signal estimates of all 12 DRT conditions were contrasted against the control condition CT in each individual subject. The resulting group map is depicted in Figure 4 C. Our second-level group analysis showed significant differences across subjects in the delay-related areas of the left and right (l/r) posterior parietal and premotor cortex that were introduced above, namely SPLl, SPLr, antIPSl, antIPSr, PMdl, PMdr. In addition, delay activity was exhibited in dorsolateral prefrontal cortex (DLPFCr), the anterior insular cortex (AICl, AICr), supplementary motor area (SMA), as well as the lobules 6 and 8 of the cerebellar hemispheres (cer6l, cer6r, and cer8r). Apart from the earlier areas in posterior parietal and premotor cortex that have been previously shown to contribute to concurrent prospective planning in monkeys (compare introduction), we also considered all other aforementioned areas as regions of interest regions (ROIs). For further details on how these ROIs were selected in individuals, please see the Method section. For each of our predefined ROI areas, we extracted GLM parameter estimates reflecting delay-related changes in fMRI BOLD signal amplitudes in different task conditions of varying planning complexity. In the following we chiefly focus on area SPLl, as an examplary ROI that has been shown to be critically involved in movement planning [15]. For results of different ROIs – contralateral cortical ROIs (left) and ipsilateral cerebellar ROIs (right) – please refer to Supplementary Figure S1. In area SPLl, delay-related GLM parameter estimates differed significantly between individual planning conditions, distinguishing both the number of potential targets ($p < 0.0001$, 2-way rmANOVA with factors condition and sequence length) and sequence length ($p = 0.001$) but there was no significant interaction of the two factors. The relative changes of the fMRI signal over time due to planning during the delay phase compared to a pre-stimulus baseline can be seen for the different conditions in Figure 4 A. As expected, the activity in SPLl was lowest during the control condition CT that does not provide any information for planning. The activity increased with the complexity of the planning problem with the highest activity for the target condition '4' with sequence length 4. As a control ROI, primary visual cortex V1l – that is supposedly not involved with motor planning – showed no such modulation (see Figure 4 B). Due to the slow BOLD haemodynamic response function (HRF), visual processes and eye movement related activity during cue presentation could influence the early delay phase of planning. Differences in pure planning activity for different task conditions in isolation are only reflected in the late delay phase. Hence, at first glance, planning related activity in SPL and in all other planning-related ROIs (compare Supplementary Figure S2 with PMdl, antIPSl, DLPFCl, AICl, cer6r, cer8r, SMA) seemed compatible with concurrent prospective planning.

Model comparison

In order to formally test our hypothesis of planning strategies during the delay phase – concurrent prospective planning (H1) against the null hypothesis of delayed planning with

Figure 3: Behavioral performance. Results are reported as the mean over subjects' individual task performance and normalized standard error (according to [29] to eliminate the between-subject variance, which does not contribute to the within-subject effect of the study). Results of the pairwise post-hoc comparisons of the respective marginal means are indicated with *** for $p <= 0.001$, ** for $0.001 < p <= 0.01$, and ns for non-significant results ($p > 0.05$). (A) Reaction times (RT) and (B) movement times (MT) were calculated as normalized averages across individual subjects' means $\pm$ SEM. Reaction times were significantly decreased for easy planning conditions ('1' and '11') compared to the control condition CT, which indicates a benefit due to planning. RT were higher in the more complex planning conditions ('2' and '4') and did not significantly differ compared to CT. Differences for varying sequence length were found for MT but not for RT. (C) Error rates averaged across subjects indicated varying task difficulty over conditions revealed by an increase of target misses for conditions with higher task uncertainty ($p = 0.001$ for 4 vs CT) and between 2- and 3-step conditions ($p = 0.002$ for 2 vs 3). (D) During the delay phase there was no significant difference between the average number of eye saccades and therefore saccades cannot explain benefit in reaction times or fMRI activity in planning-related areas.

Figure 4: fMRI activity related to motor planning. (A) Time course of fMRI activity as percentage of signal change normalized to pre-stimulus baseline and delay-activity estimates (beta parameter from GLM) in each planning condition in planning related area SPLl show increasing planning-related BOLD amplitudes with increasing task complexity. We report across-subjects averages and within-subjects variance as the normalized standard error (according to [29]). Time course activity and GLM estimates of further ROIs – contralateral cortical ROIs (left) and ipsilateral cerebellar ROIs (right) – are provided in Supplementary Figure S1. Average MNI-coordinates (x, y, z in mm) are provided for each ROI. Statistical results are indicated with *** for $p <= 0.001$, ** for $0.001 < p <= 0.01$, * for $0.01 < p < 0.05$, and ns for non-significant results ($p > 0.05$). (B) In a 'non-planning ROI' (V1l) BOLD signal changes were not significantly different between conditions. (C) Second-level activation map shows significant delay-related fMRI activity across subjects in planning related areas (see Results for details) when contrasting DRT conditions vs. the control condition CT ($p \geq 0.05$ family-wise error FWE-corrected for multiple comparisons).

uncertainty reduction only based on past sensory information (H0) – we compared the fMRI activity modulation over different experimental conditions to the expected information modulation determined for both hypothesis from an optimal decision-making model with information constraints (see Figure 2). For a detailed description of both hypothesis please see the Methods section. Assuming motor planning during the delay phase only in terms of uncertainty reduction based on memorized information of the perceived cue stimulus, the decision-maker requires information cost I_1 to first update the internal memory. Correspondingly the action uncertainty gets reduced from a prior over all actions to a posterior over potential actions given the memory, which requires an additional information cost I_2. We contrasted this null hypothesis H0 with the assumption of concurrent prospective planning, where separate action plans are made for all potential targets. In this alternative hypothesis H1, the memory update is identical to H0 (same information cost I_1), but the information cost required for the reduction of uncertainty over actions is now composed of the sum of information costs to form each possible motor plan (I_2). The exact amounts of information (I_1 and I_2) depend on the capacity of the information channels defined by model parameters $beta_1$ and $beta_2$ for the memory and the action process. Three example profiles of information modulation with different capacities are shown in Figure 2 C.

To find out which hypothesis explains our data best, we established (non-negative) multilinear regressions between the fMRI activity modulation during the delay period and the two information modulations predicted by each of the two hypotheses. For both hypotheses, we first calculated the expected information costs for possible settings of information capacities and we regressed these theoretical information modulations with the respective subject-specific GLM activity estimates over the 12 DRT conditions for all ROIs separately. Figure 5 A shows, exemplarily for brain area SPLl, the R^2-values of the regressions for the best fitting information capacities for each subject under the two hypotheses (which we refer to as bounded in the Figures 4 and 5). A within-subject comparison of the R^2-values for the two hypotheses showed that the information profiles under the prospective planning hypothesis H1 provide a significantly better explanation of the fMRI modulation than the delayed planning hypothesis H0 in SPLl (SPLl: $p < 0.0001$ rmANOVA) as well as in all other planning related ROIs, but not in control ROI V1l (compare Supplementary Figure S2). For further details on the statistical analysis see the Methods section. Moreover, we applied a nested model F-test statistic to both hypotheses to find out whether the predicted planning-specific information I_2 contributed significantly to the multilinear regression of the fMRI signal. We found that for most of the subjects (15 from 19 for SPLl) under the prospective planning hypothesis H1 the planning information I_2 improved the regression of the signal modulation significantly (see Figure 5). In contrast, the nested model tests for H0 revealed that model regressions did not improve significantly by taking I_2 into account.

To address the question in how far concurrent planning is limited in its capacity, we compared the R^2-values of the regression with an optimal decision-making model without capacity bounds that we obtain from the bounded decision-making model as a limit case of maximum capacity (which we refer to as not-bounded in Figures 4 and 5). We found that the correlation of measured brain activities in SPLl as well as in all other planning related ROIs was significantly increased for model predictions with subject-individual bounds (SPLl: $p < 0.0001$ rmANOVA, compare Supplementary Figure S2 for all other ROIs) compared to an unbounded maximum capacity model. This suggests that judging from the modulation of the fMRI signal alone, it seems that subjects were limited in their information processing. As a control, the R^2-value of the information

Figure 5: Model comparison. (A) R^2-values of the regressions for the best fitting information capacities for individual subjects for H0 and H1 are compared to not-bounded models. (B) Resulting theoretical quantitative predictions of the expected information costs and expected utility over all task conditions are plotted for individual subjects. Expected values of information costs $E[I_1]$ and $E[I_2]$ of subjects' bounded model fits to the fMRI correlates was lower than for not-bounded model (blue lines). This gives hint to prospective planning activity with subject-individual planning capacities.

modulation in primary visual area V1l was close to zero (see Supplementary Figure S2). The individually fitted information bounds under the two hypotheses H0 and H1 can be seen in the 3d graphs shown in Figure 5 B. The expected information costs over all conditions $E[I_1]$ and $E[I_2]$ of subject-individual best model fits were lower compared to the predicted information boundaries $E[I_1]$ and $E[I_2]$ when assuming no bounded information capacities for I_1 and I_2 (blue lines). Our comparison of the expected information values for the bounded and not-bounded model indicated, that for all subjects mainly information capacity for prospective planning I_2 was reduced whereas information for memory I_1 was reduced but still closer to the predictions of the model with the not-bounded assumption. Expected information values for subject-specific model fits to activity in all other ROIs can be found in the Supplementary Material (Table 1 - Table 4). Assuming a simple 0/1-utility function U for our task (see Methods), the expected utility $E[U]$, shown on the z-axis, was individually different for the decision-making models and is higher for subjects with higher capacity limits for I_1 and I_2.

To finally investigate the impact of limited information processing for concurrent prospective planning in individual task conditions with different complexity (i.e. number of potential targets and sequence length), we illustrated frequencies of information costs I_1 and I_2 for subjects' best model fits in a histogram representation for each condition (see Figure 6). We contrasted the frequency distributions with the information predictions for a perfect decision-maker without information processing bounds (blue line). Deviations from the information with maximal capacities show evidence for bounded planning. It can be seen that subjects generally lie below the information bound of the perfect decision-maker.

Figure 6: Theoretical expected information costs I_1 (left) and I_2 (right) of prospective planning is based on model parameters determining memory and planning capacities fitted for all individual subjects (hypothesis H1 "bounded"). Histograms represent the frequency distributions of the information costs, dependent on task conditions. Information values varied between bounded model predictions regressed to subjects fMRI data compared to the model predictions in the not-bounded case (in blue). Note that generally subjects lie below the information cost of the not-bounded decision-maker and only for the most simple 2-step conditions subjects' information costs for memory (I_1) deviate in the different direction from the predictions in the not-bounded case. This results from the specific task design and the fact, that bounds are provided on the total expected information. Decision-makers with not-bounded planning capacities can optimally assign resources to more difficult conditions and save memory costs for 2-step conditions, because no uncertainty about the target location will remain when s_2 is revealed given that all actions are planned prospectively under a high information resource for I_2.

3 Discussion

Using fMRI and information-theoretic modeling, we have investigated neural correlates of information processing costs during concurrent motor planning in the human motor system [15]. We manipulated informational complexity of movement planning by varying both the temporal extension of the movement sequence length as well as the degree of concurrency (the number of potential targets). We compared how much of the variance of the fMRI signal could be explained when assuming concurrent prospective planning for multiple potential targets (hypothesis H1) and when assuming no prospective planning, but only uncertainty reduction based on past sensory information (hypothesis H0). We found that the information costs of concurrent prospective planning explained fMRI profiles across conditions significantly better than assuming a simple memory hypothesis (delayed planning) that delays all anticipatory planning activity into the future until a second sensory stimuli (the go-signal) will resolve the remaining uncertainty. Our results therefore add to a growing body of evidence that suggests the use of concurrent prospective planning in the parietal-frontal planning system when faced with multiple potential futures [30, 31, 7, 8, 32, 33, 9, 2, 34].

While the parallel planning of multiple potential futures comes with a reaction time advantage whose behavioral consequences could be positively selected by evolution, it is also immediately clear that it cannot scale to scenarios with arbitrarily large amounts of uncertainty due to an excessive computational burden. Therefore, one would naturally expect a trade-off between the degree of concurrency in motor planning and the amount of information processing required. Evidence for such a trade-off has been previously reported in behavioral studies [35], where it has been shown that competition between movement plans increases motor variability, thus suggesting a shared resource for movement planning. In our experiment, this could be seen both in the behavior and the fMRI BOLD signals. Behaviorally, we noted an increased error rate for conditions with high degree of concurrency, suggesting a limitation in precision for concurrent planning. Neurally, we found that the best model correlates are characterized both by the assumptions of concurrent planning and limited information capacity. In particular, we found in our nested model analysis for the two information profiles regarding memory and planning that adding the planning information significantly improved the variance explained in the fMRI signal.

Serial vs. parallel processing The null hypothesis H0 has been aligned with more traditional theories of sensorimotor processing whose point of view is that perceptual, cognitive and motor processes take place successively and only a single motor program is prepared in the end [5, 6]. For our experiment that means that during the delay phase one could only reduce uncertainty about the specification of that motor program to a certain extent, based on the memory of the pre-cued information from the first stimulus cue s_1. The full specification of the motor program would have to be postponed until the end of the delay phase. Since the presence of more possibilities goes hand in hand with less uncertainty reduction, this hypothesis would predict less planning activity in multi-target conditions, whereas the concurrent planning hypothesis would predict increased activity in multi-target conditions. A direct comparison with fMRI activity is, however, confounded by persistent activity related to memory in both cases. Avoiding such a memory confound by showing the stimulus directly, would instead have produced a stimulus confound. Accordingly, we have conducted a bivariate regression of the fMRI signal for the expected amount of information processing for memory and planning. This

regression analysis significantly favoured the concurrent planning hypothesis H1.

Previous neural studies that have favored the hypothesis of concurrent motor planning have been mostly conducted in monkeys. Cisek and colleagues [31] have found, for example, that PMd activity in a two-target condition reflects presence and relative location of both targets, and that once the right target is indicated by a nonspatial cue, the corresponding directional signal is increased, while the other one is suppressed, thus, suggesting two concurrent motor plans vying for execution. Similarly, Klaes and colleagues [9] have found that neurons in the frontoparietal reach areas of monkeys simultaneously represent two different movements associated with two different sensor-action rules, when it was made unclear to the monkey which of the rules to apply. In a similar vein, Cui and colleagues [2] have found in a nonspatial effector choice task (saccade vs. reach) that the parietal reach region encodes both potential action plans, whereas the dorsal area 5d only reflected the ultimately selected effector. A recent fMRI study [34] also reported supportive evidence for the affordance competition hypothesis in humans, demonstrating that task-relevant information biases activity of primary motor regions before movement onset and that coupling with fronto-parietal regions increased when the evidence for competing actions was similar. Other studies that have supported the affordance competition hypothesis in humans have mostly concentrated on behavioral features suggestive of concurrent planning [36, 12].

Other studies [1, 37, 38] have argued that decisions between different options are made upstream in prefrontal brain areas and are independent of the particular sensorimotor contingency of the task, arguing against the notion of concurrent action planning. However, decisions in these tasks usually involve choices between goods (e.g. apple vs. banana), where the effector is not directly relevant for the choice, even though different action costs can be integrated within the valuation of different options [37]. This is in contrast to action-based decisions like in our study, where the choice is tightly linked with the effector through the spatial nature of the stimuli. Our study clearly falls in the latter category and fits with previous results on concurrent planning. In how far these results can be generalized to decisions between nonspatial stimuli with different values is an open question that might require the careful comparison of different stimulus and task designs.

In contrast to neurophysiological studies in monkeys that showed the representation of multiple action plans in PCC and PMd Cisek2005b, Klaes2011, we additionally describe such representation also in other brain areas such as the SMA, the DLPFC, the antIPS and the cerebellum. Moreover, we further explain the activity modulation in all aforementioned areas with a normative information theoretic bounded rationality model.

Limitations in memory and planning In our study we have investigated limitations of concurrent planning in terms of the number and the sophistication of multiple plans. Limitations in parallel motor performance have been previously studied in dual-task designs. Considering the cognitive costs of dual task performance, serial processing frameworks [39, 40] were originally proposed that aim to explain delayed reaction times for secondary tasks [41]. Accordingly, the Response Selection Bottleneck (RSB) model [42] assumes that the crucial limitation (or bottleneck) in dual-task performance is located in the response selection stage. In contrast, capacity sharing models [43, 44] allow for sharing of cognitive resources in the central processing stages of two tasks. By manipulating task features like stimulus onset asynchrony and no-go trials, it has also been argued that subjects can somewhat switch between serial and parallel processing strategies [45, 46, 47, 48, 49].

As demonstrated in the current study, our information-theoretic model assumes con-

strained information processing for action planning and could be adapted to either delayed planning or concurrent prospective planning scenario, to allow for a quantitative analysis. Another important limitation is imperfect memory of the stimulus during action planning. The concept of working memory as a short-term active storage of information [50] relates to the idea of a limited capacity control process involved in keeping or discarding information [51]. Quantifying the limited information capacity of working memory has been addressed in numerous studies, for example on visual working memory [16, 18, 19, 20, 52, 21] and spatial working memory [23, 24, 53, 54] with growing evidence that they share a common resource limitation [55, 56]. In terms of neurophysiology, it has been suggested early on, that memory limitations can be considered as the result of the limited computational capacity of single neurons [57]. In our model, we have represented limitations of working memory more abstractly, by an internal variable that can only assume a finite amount of values and whose precision is curtailed by a corresponding information constraint. This abstraction is based on the idea that any information processing limitation can ultimately be thought of as a limitation in the amount of uncertainty that can be reduced [58].

Information theory, behavior and neural signals   Our study belongs to a large family of investigations that have used information theory to quantitatively model information processing constraints in behavior and neural signals. In behavioral experiments information capacity limits have been established for working memory, attention, perceptual identification, decision-making, motor planning and execution [16, 59, 60, 26]. Informational complexity in behavioral tasks is often related to reaction or movement times and task accuracy. The most well-known examples of this are Hick's law that relates reaction time linearly to the entropy of a choice stimulus and Fitts' law that relates movement time to an index of difficulty measured in bits [61, 62]. However, similar approaches have also been used to estimate the capacity for cognitive control depending on the entropy of the stimulus [63]. In our task, reaction times and error rates increased with higher task complexity, as expected from previous studies on motor sequence learning [3]. However, directly relating this change in reaction time to information complexity of our two hypotheses is confounded, because it is not clear whether the increase in reaction time during the response phase stems from a more complex decision between different ready-made motor plans (H1) or whether the increase results from finishing a single motor plan based on the incomplete uncertainty reduction during the delay phase (H0).

Importantly then, by going beyond the behavioral analysis, we could use the different information profiles for concurrent and serial planning to regress the fMRI signal. However, simply applying information-theoretic concepts to brain signals without taking into account the behavioral task, would not have been enough to distinguish between the two hypotheses. Previous neurophysiological studies have, for example, used mutual information between stimuli/behavior and neural signals to establish a neural code either for encoding or decoding [64], quantified the richness of conscious states within a theory of integrated information [65], or related activity in distinct regions of the prefrontal cortex to sensorimotor and cognitive control [66, 67]. A considerable number of imaging studies have also found neural correlates of informational surprise in sensory areas of the brain [68, 69, 70] related to prediction error in the context of predictive coding theory, with a wide range of applications ranging from action understanding in the mirror neuron system [71, 72, 73] and value-based decision-making [74] to hierarchical motor control [75]. However, in order to go beyond information-theoretic quantification of neural signals we need to consider both information constraints and task-related constraints [76].

Bounded rationality In contrast to many previous studies that have relied on information theory to estimate neural processing capacity, we have employed a class of bounded rationality models that trade off both utility and information processing costs [77, 78, 79, 80, 81], similar to the rate distortion trade-off in information theory [82] that defines relevant information when bandwidth is limited. Such a generalized trade-off makes this class of models applicable to tasks with arbitrary utility function. Moreover, using information constraints on multiple variables, we can design optimality models that simultaneously explain behavior and optimal information flow between internal variables that can be correlated with fMRI BOLD signals. In previous behavioral studies, the trade-off between utility and information has been used in the context of rational inattention and quantal response equilibria in economic decision-making [83, 84], perceptual representation in identification and memory tasks [60, 85], reaction time and endpoint variability for motor planning under time constraints [26], abstraction in sensorimotor processing [27], decision-making by sampling [86] and planning in a Markov environment [87, 88].

Similar to these previous studies where behavioral task performance and information processing capacities were measured, we here use a normative probabilistic optimality model for uncertainty reduction and parallel processing. In this study, however, we go a step further and relate the predicted information flow with fMRI activity during motor planning. In particular, measuring the activity of premotor and parietal planning areas during the delayed response tasks allowed us to measure planning capacity for movement preparation. As the bounded rationality framework allows for multiple information constraints including internal variables for memory and action planning, we could regress fMRI activity with respect to these different information quantities and we could test the hypothesis of concurrent prospective planning (H1) against the null hypothesis of mere uncertainty reduction (H0). This approach rests on the assumption that brain signals reflect at least approximately an optimal information flow – an assumption that has been applied very successfully in the past, for example in the context of sparse coding [89, 90]. Ultimately, it is an empirical question for future studies, how far this class of models can be developed in their explanatory power, but they open a new exciting avenue that allows relating both behavior and neural representations to optimal information processing assumptions.

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5   Author contributions

S.S., A.L. and D.A.B. designed the experiment; S.S. and A.L. developed the experimental setup and acquired data; S.S., D.A.B. generated theoretical predictions from computer simulations; A.L., D.A.B supervised the project; S.S., A.L. and D.A.B. wrote, discussed and edited the manuscript.

6   Declaration of interests

The authors declare no competing interests.

7 Methods

Experimental Methods

Subjects Nineteen right-handed healthy subjects (11 females, 8 males) in the age range of 22 and 41 years (mean = 27.5, SD = 4.5) participated in the experiment and were included in further data analysis. Initially, we recruited 22 subjects, but data of three subjects was excluded because of strong movement artifacts. Participants provided written informed consent in accordance with the declaration of Helsinki and the study was approved by the ethics committee of the University Hospital and the Faculty of Medicine at the University of Tübingen.

Experimental Paradigm. We employed a delayed response task (DRT), in which subjects were instructed to generate sequences of key presses with four possible keys to control right, left, up, and down of a cursor movement. Each trial started with a random fixation phase of 13.5 - 16 sec (FIX), where a fixation cross was presented in the middle of the four fields and should be fixated with the eyes. This fixation period was followed by three principle task phases: cue presentation, delay/planning and response. In the cue presentation phase, subjects were shown one or multiple potential targets (four different target planning conditions $c_T \in \{$'1', '11', '2', '4'$\}$ as detailed below) with one of three possible sequence lengths (three different step conditions $c_S \in \{2, 3, 4\}$). The timeline of a DRT is illustrated in Figure 1.

Cue presentation phase. The display area is divided into four panels each made up of 3x5 fields as shown in Figure 1 A). Each field represents a target position that can be reached with a cursor. Panels could be surrounded by a frame, which indicated that the highlighted target position within the frame should be taken into consideration as a potential target for motor planning. In all trials (including the training phase), only target positions with a sequence length of 2, 3 or 4 were considered due to the step conditions $c_S \in \{2, 3, 4\}$ of the experimental design. The potential target positions were always shown for 3 sec (CUE). Depending on the target planning condition, there were four different kinds of cues:

- '1'-Target Planning Condition: In this one-fold planning condition only one panel was framed containing a single highlighted potential target location that always corresponded to the actual target location in the response phase.

- '11'-Target Planning Condition: In this two-fold planning condition there was also a single framed panel that contained two potential targets highlighted, only one of which was selected as the actual target during response phase.

- '2'-Target Planning Condition: In this two-fold planning condition, two panels were framed, each containing a single highlighted potential target from which one was selected for execution.

- '4'-Target Planning Condition: In this four-fold planning condition all four panels were framed, each containing a single potential target highlighted for planning, from which one was selected in the response phase.

Cue presentation was followed by a mask of 1 sec (MASK), which was intended to "overwrite" any after-images of the cue.

Planning phase. The planning phase was a delay phase of 14 - 16.5 sec (DEL) following the mask to allow subjects to plan one or multiple movement paths based on the

information they obtained from the visual target cues. During this time, only a fixation cross was displayed in the center of the screen. From trial start to the completion of the planning phase, subjects had to keep their finger in rest position and where therefore asked to press the central button of the input device.

Response phase. In the response phase (RES), the actual target was determined from the set of potential targets and a go-signal. This go-signal comprised a half-size-frame encompassing six fields (including the actual target) was displayed around one half of one of the four field panels, however, the correct target itself was not highlighted in any way. Accordingly, the correct target field could only be uniquely identified through this go-signal if subjects remembered the appropriate information from the previously displayed target cues. Subjects were instructed to perform the movement sequence towards the inferred target field as fast and directly as possible within the allowed time window of 3 sec (otherwise the trial was terminated with an incomplete response). Depending on the distance of the target (sequence length), only the first 2, 3 or 4 key presses were considered before the trial was terminated. Subjects could observe the corresponding cursor movement and got immediate visual feedback of their performance at the end of the trial, by highlighting the cursor position in green (red) when the final reached position was correct (incorrect).

Besides DRT trials, we also included control trials (CT) in which no planning was possible during the delay phase. Like the other DRT trials, control trials were comprised an initial fixation phase and the three principal task phases – cue presentation, planning and response. Different to the DRT, however, in the cue presentation phase, no targets were highlighted. Hence, subjects were not informed about any potential target location and therefore could not plan specific movements during the delay planning phase. In the response phase, the actual target was indicated directly by highlighting the corresponding target field, so that the movement sequence to reach the target could only be planned once the actual target location was revealed.

Our experiment usually consisted of four blocks of 30 trials each (one subject had five blocks, two subjects only three blocks) typically resulting in a total of 120 trials. The overall experiment lasted ~ 80 min per subject. Each block consisted of 6 control trials and 6 trials for each target planning condition. Moreover, the 6 trials had an equal share of step conditions, i.e. 2 trials with sequence length of 2, 3, and 4, respectively. The order of the trials in any given block was permuted randomly.

In our experimental setup we used a Windows 7 based computer with R2007b (The MathWorks, Inc.) and the Cogent Graphics Toolbox (developed by John Romaya at the LON at the Wellcome Department of Imaging Neuroscience) to generate the visual stimuli for the experimental trial sequences and to record and store subjects' behavioral responses and all relevant information associated with the visual stimuli sequence. The visual stimuli were back-projected by an LCD projector (1024x768 pixels; 60 Hz refresh rate) onto a semi-transparent screen at the end of the scanner bore behind the head coil. Subjects viewed the screen via a mirror that was mounted on top of the head coil. Screen dimensions amounted to 28 deg x 37 deg visual angle.

Behavioral performance monitoring The instructed finger movements were monitored using the 5 Button Diamond Fibre Optic response device (Current Design, Philadelphia, US) operated by repetitive thumb flexions. From this we could extract reaction and movement times as well as error rates defined by the frequency of target misses.

For all behavioral analysis, we excluded trials, when movements were not initiated (1%) to compute reaction times and error rates and trials, when movements were not

initiated or completed (2%), to compute movement times.

Additionally, eye movements were monitored at 50 Hz sampling rate throughout the scanning sessions using an MRI-compatible eye camara and infra-red illumination system (SMI SensoMotoric Instruments) and Viewpoint Eye Tracker software (Arrington Research, Scottsdale, US). Eye position recordings were filtered using a 10 Hz Chebyshev Type II low-pass filter. Saccades were detected using an absolute velocity threshold of 30 °/s (for a single recording of one subject 40 °/s). Eye data from 2 subjects were excluded from the analysis because of incompleteness.

We performed 2-way repeated measures ANOVAs (rmANOVA) with the factor target condition ('1', '11', '2', '4' and CT) and factor sequence length (2, 3, or 4) for the behavioral analysis of reaction times, movement times, error rates and saccades. In addition we applied pairwise post-hoc comparisons of the respective marginal means. For this and all other rmANOVAs we tested for sphericity (Mauchly's test) and applied the Greenhouse-Geisser correction whenever the assumption of sphericity was violated.

MRI image acquisition and analysis   MRI images were acquired on a 3 T Siemens PRISMA scanner (Siemens, Ellwangen, Germany). A T1-weighted magnetization prepared rapid-acquisition gradient echo (MP-RAGE) structural scan (176 slices, 256x256 voxel resolution, 1x1 mm inplane voxel size, slice thickness = 1 mm, gap = 0 mm, repetition time = 2300 ms, echo time = 2.96 ms, field of view = 256 mm) was obtained in parallel to the task training. Functional T2*-weighted gradient-echo planar imaging (EPI) volumes (48 sclices, 64 voxel resolution, 3x3 mm inplane voxel size, slice thickness = 3 mm, gap = 0 mm, repetition time = 2000 ms, echo time = 35 ms, field of view = 1344 mm, flip angle=75 deg) completely covered the cerebellar cortex as well as subcortical structures. Per subject we obtained 600 EPIs during a single session of 19.75 min length, resulting overall in 2400 EPIs for 16 of the subjects (1800 and 2177 for prematurely terminated recordings and 3000 for a subject with an extra-session). Functional image processing was conducted with the SPM12 software package (Wellcome Centre for Human Neuroimaging, London, UK, Matlab 2016a Release) and included spatial realignment of all functional images to the first EPI image as a reference, co-registration of the anatomical T1 image and the mean functional EPI image, spatial normalization to the Montreal Neurological Institute space (MNI-template) with voxel size of 1x1x1 mm^3 for T1 and 3x3x3 mm^3 for EPI images and spatial smoothing of the normalized EPIs with a Gaussian kernel (7 mm full-width at half maximum (FWHM) Gaussian filter.

Functional fMRI analysis was first performed on an individual level (first-level analysis) and then on the group level (second-level analysis). The subject-specific analysis of fMRI BOLD activity is based on a general linear model (GLM). To this end for each session we specified 5 boxcar regressors for the cue phase of 3 sec (CUE) for each of the four target planning conditions (c_T) and the control condition, as well as 5x3 boxcar regressors both for the delay phase of 14 - 16.5 sec (DEL) and for the response phase of 3 sec (RES), namely for each of the four target planning conditions (c_T) and the control condition and separately for each of the three step conditions (c_S). All aforementioned boxcar regressors were convolved with the canonical hemodynamic response function in SPM12. In addition, the 6 motion parameters from the realignment procedure were additionally included as regressors of no interest. The fixation phase was not explicitly modeled and served as an implicit baseline. Each experimental session therefore was modelled separately with 41 regressors for each subject (5 x CUE + (5*3) x DEL + (5*3) x RES + 6 x motion regressors).

Regions of interest (ROIs) were selected as brain areas that exhibited significant

planning-related activity in the DRT conditions compared to the control-task across subjects. Given the estimated regressor parameters of the GLM, in the 2nd-level analysis, we first determined significant voxels whose t-values for the contrast of interest (DRT_{Delay} > CT_{Delay}) were below a threshold of $p < 0.05$ (t-test across subjects' first level contrast images for DRT_{Delay} > CT_{Delay} family-wise error FWE-corrected for multiple comparisons). We found significant bilateral activities in brain areas typically involved in motor planning and visual memory [15]: posterior parietal cortex (superior parietal lobule (SPL) and anterior intraparietal sulcus (antIPS)), dorsal premotor cortex (PMd), dorsolateral prefrontal cortex (DLPFC), anterior insular cortex (AIC), cerebellum in lobulus VI and VIII (cer6 and cer8) and supplementary motor area (SMA). As a group coordinate of a ROI, we selected those voxel coordinates that were characterized by a maximum t value in the group analysis. Accordingly, we defined 15 group coordinates for the aforementioned areas (note that for the SMA, functional activity could not reliably be associated with either left or right hemisphere and therefore we only defined a single ROI). Also, we included left primary motor cortex (M1l) due to its contribution for our task related finger movements of pressing a button and therefore to control for activity related to movement execution directly. Similarly, to control for stimulus related activity we included left primary visual cortex (V1l). We identified the two anatomical regions of primary visual cortex (V1l) and primary motor cortex (M1l) with the corresponding group contrasts (CUE>0) and (RES−CUE; this was to account for the visual information present in the response phase).

For each individual subject, we mapped group ROI coordinates to individual ROI coordinates. This was done for each ROI, namely by identifying the coordinates of the local statistical maximum in the subject-specific first-level contrast (DRT_{Delay} > CT_{Delay}) that was closest to the group-coordinates.

Group MNI coordinates of all 17 defined ROIs together with the average spatial dispersion of the ROI center on the individual subjects can be found in Supplementary Table 5.

For each subject and ROI, we extracted the GLM mean model parameters for the regressors of interest from a 3 mm radius sphere around each individual ROI coordinate. These beta parameters were (session-wise) normalized to the residual beta for any given session (i.e. baseline) to provide an estimate of the %-signal change of the fMRI signal. We computed rmANOVAs over fMRI beta estimates with factor target planning condition ('1', '11', '2', '4') and with factor sequence length (2, 3, 4). In addition, event-related time courses of the fMRI-signal time courses (ERTs) of signal intensities were extracted using NERT4SPM [15].

Theoretical Methods

Bounded Rationality Model We applied the information-theoretic bounded rationality framework [25, 91] to our experimental task, where information about the hidden world state $w \in \mathcal{W}$ (the exact target location) is revealed in two steps, first by the initial cue stimulus $s_1 \in \mathcal{S}_1$ indicating all possible target locations, and after a delay by the go-signal $s_2 \in \mathcal{S}_2$ that resolves the remaining uncertainty about the actual hidden target w. After seeing the cue stimulus, the agent can form a memory $m \in \mathcal{M}$ during the planning delay phase, before perceiving the cue stimulus s_2 and subsequently selecting an action $a \in \mathcal{A}$ that corresponds to a movement sequence leading to a target location. The sets $\mathcal{W}$, $\mathcal{S}_1$, $\mathcal{S}_2$, $\mathcal{M}$ and $\mathcal{A}$ are finite and discrete, with $|\mathcal{W}| = 40$ possible target locations (in distance of 2,3 or 4 steps), $|\mathcal{A}| = 80$ possible movement sequences, $|\mathcal{S}_2| = 8$ possible half-sized frames for each panel and $|\mathcal{S}_1| = |\mathcal{M}| = 820$ possible combinations of potential

targets over all conditions. For any particular target condition c_T and step condition c_S, we then get a uniform distribution over stimuli

$$p(s_1|c_T, c_S) = \begin{cases} \frac{1}{N_{c_T, c_S}} & \text{if } s_1 \in \mathcal{S}_{c_T, c_S} \subset \mathcal{S}_1 \\ 0 & \text{otherwise} \end{cases} \tag{1}$$

where $\mathcal{S}_{c_T, c_S}$ is the subset of stimuli that belong to the condition (c_T, s_T) and $N_{c_T, c_S} = |\mathcal{S}_{c_T, c_S}|$ is the number of stimuli in that condition, where $N_{1,2} = 8$, $N_{1,3} = 16$, $N_{1,4} = 16$, $N_{11,2} = 4$, $N_{11,3} = 16$, $N_{11,4} = 16$, $N_{2,2} = 24$, $N_{2,3} = 96$, $N_{2,4} = 96$, $N_{4,2} = 16$, $N_{4,3} = 256$, and $N_{4,4} = 256$. The marginal distribution over stimuli is given by $p(s_1) = \sum_{c_T, c_S} p(c_t, c_S) p(s_1|c_T, c_S)$ where all conditions are equally likely with $p(c_T, c_S) = \frac{1}{12}$. As the second stimulus s_2 surrounds any potential target from s_1 with a rectangular half-frame, the distribution $p(s_2|s_1)$ is a uniform with non-zero probability over a single value of s_2 when $c_T =$'1', two possible values of s_2 when $c_T =$'11' or $c_T =$'2', or four possible values of s_2 when $c_T =$'4'.

In the model, the agent chooses the action a to maximize the task utility $U(w, a)$ under the constraint that only a certain amount of information-processing can be achieved when forming the memory m and selecting the action a. For our task the utility function U is a simple 0/1-utility: it is 1 whenever the action a is compatible with the hidden target w and 0 otherwise.

Since information-processing can be unreliable, the agent's memory state and action policy are formalized by probability distributions $p(m|s_1)$ and $p(a|m, s_2)$, such that the amount of information processing can be captured by the Kullback-Leibler divergence between the prior distributions $p(m)$ and $p(a)$ and the posterior distributions $p(m|s_1)$ and $p(a|m, s_2)$, respectively. The bounded rational decision-making problem can then be written as a constrained optimization problem

$$\max \left\{ {}_{p(a|m, s_2), p(m|s_1)} E[U] - \frac{1}{\beta_1} I(M, S_1) - \frac{1}{\beta_2} \left(I(A; M) + I(A; S_2|M) \right) \right\}. \tag{2}$$

where the expectation is taken with respect to the distribution

$$p(w, s_1, s_2, m, a) = p(w|s_1, s_2) p(s_1) p(s_2|s_1) p(m|s_1) p(a|m, s_2), \tag{3}$$

with $p(s_1)$, $p(s_2|s_1)$ and $p(w|s_1, s_2)$ defined by the task, and $p(m|s_1)$ and $p(a|m, s_2)$ left for optimization. The information quantities $I(M, S_1)$ and $I(A; M) + I(A; S_2|M)$ respectively measure the average Kullback-Leibler divergence between the distributions $p(m)$ and $p(m|s1)$ for memory formation and the average Kullback-Leibler divergence between the distributions $p(a)$ and $p(a|m, s_2)$ for generating a specific action given memory m and stimulus s_2. The parameters β_1 and β_2 reflect the degree of boundedness, where $\beta_{1,2} \to \infty$ reproduces a Bayes-optimal maximum expected utility decision-maker. The bounded optimal solution for equation 2 is given by

$$\begin{cases} p(m|s_1) \propto p(m) e^{\beta_1 \Delta F(m, s_1)} \\ p(m) = \sum_{s_1} p(s_1) p(m|s_1) \\ p(a|m, s_2) \propto p(a) e^{\beta_2 \sum_w p(w|m, s_2) U(w, a)} \\ p(a) = \sum_{s_1, s_2, m} p(a|m, s_2) p(m|s_1) p(s_2|s_1) p(s_1) \end{cases} \tag{4}$$

with

$$\Delta F(m, s_1) = \sum_{a, s_2, w} p(a|m, s_2) p(s_2|s_1) p(w|s_1, s_2) U(w, a) - \frac{1}{\beta_2} \sum_{a, s_2} p(a|m, s_2) p(s_2|s_1) \log \left(\frac{p(a|m, s_2)}{p(a)} \right)$$

and with $p(w|m, s_2)$ determined from equation 3.

Modelling information-processing during Delay Phase. If we want to apply equation (4) to model planning during the delay phase, we have to be aware that the decision rule $p(a|m, s_2)$ requires the agent to know the go-stimulus s_2 when deciding about the action a, an information that is not available during the delay period. We consider two hypotheses for information-processing during the delay phase.

- Hypothesis 0: Delayed Planning. Planning of the action a according to $p(a|m, s_2)$ is delayed until the response phase, once s_2 is known. The delay phase is only used for uncertainty reduction, modeled by the mathematical transition from the prior $p(m)$ to the posterior $p(m|s_1)$ and in the space of actions from $p(a)$ to $p(a|m)$. In any particular condition (c_T, c_S), we would then expect the information costs

$$I_1(c_T, c_S) = \sum_{s_1} p(s_1|c_T, c_S) \sum_m p(m|s_1) \log \frac{p(m|s_1)}{p(m)} \tag{5}$$

$$I_2(c_T, c_S) = \sum_{s_1} p(s_1|c_T, c_S) \sum_m p(m|s_1) \sum_a p(a|m) \log \frac{p(a|m)}{p(a)} \tag{6}$$

  for memory formation and action processing respectively, and the average over all conditions given by
  $\sum_{c_T, c_S} p(c_T, c_S) I_1(c_T, c_S) = I(M; S_1)$ and
  $\sum_{c_T, c_S} p(c_T, c_S) I_2(c_T, c_S) = I(A; M)$.

- Hypothesis 1: Prospective Planning. Once the uncertainty over actions is reduced to $p(a|m)$ by observing s_1, all possible s_2 are anticipated in the delay phase, and for each s_2 an action is planned according to $p(a|m, s_2)$. Depending on available information resources, the plans can be more or less precise. Once the actual go-stimulus s_2 is revealed during the response phase, one of the planned actions can be immediately carried out. During the delay phase in any particular condition (c_T, c_S), we would then expect the information costs

$$I_1(c_T, c_S) = \sum_{s_1} p(s_1|c_T, c_S) \sum_m p(m|s_1) \log \frac{p(m|s_1)}{p(m)} \tag{7}$$

$$I_2(c_T, c_S) = N_{T,S} \sum_{s_1} p(s_1|c_T, c_S) \sum_m p(m|s_1) \sum_{s_2} p(s_2|s_1) \sum_a p(a|m, s_2) \log \frac{p(a|m, s_2)}{p(a)} \tag{8}$$

  for memory formation and action processing respectively, with $N_{1,S} = 1^2$, $N_{11,S} = 2^2$, $N_{2,S} = 2^2$ and $N_{4,S} = 4^2$, and the average over all conditions given by
  $\sum_{c_T, c_S} p(c_T, c_S) I_1(c_T, c_S) = I(M; S_1)$ and
  $\sum_{c_T, c_S} \frac{1}{N_{T,S}} p(c_T, c_S) I_2(c_T, c_S) = I(A; M) + I(A; S_2|M)$.

Assuming a linear relationship between informational surprise and brain signal fMRI(c_T, c_S) for each condition (c_T, c_S), we get a linear regression model

$$\text{fMRI}(c_T, c_S) = \alpha_1 I_1(c_T, c_S) + \alpha_2 I_2(c_T, c_S) + \alpha_0,$$

with model parameters α_i, $i = 0, 1, 2$.

For each of the two hypothesis H0 and H1, we tested the multilinear regression between the fMRI activity modulation and the two information modulations predicted by the models, and with a nested model F-statistic ($\alpha = 5\%$), to find if I_2 significantly improves the regression. Therefore, we applied the statistical test to the models with subject's individual best fitting capacities and for individual fMRI activities in all relevant ROIs.

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