Title: Single voxel autocorrelation uncovers gradients of temporal dynamics in the hippocampus and entorhinal cortex during rest and navigation

Authors: Nichole R. Bouffard*[1,2], Ali Golestani*[1], Iva K. Brunec[3], Buddhika Bellana[1,4], Morgan D. Barense†[1,2], Morris Moscovitch†[1,2]

* These authors contributed equally

† Shared senior authorship

Affiliations

[1]Department of Psychology, University of Toronto, Toronto, Ontario, Canada

[2]Rotman Research Institute, Baycrest Health Sciences, North York, Ontario, Canada

[3]Department of Psychology, Temple University, Philadelphia, Pennsylvania, USA

[4]Department of Psychology, Glendon College - York University, Toronto, Ontario, Canada

Abstract

During navigation, information at multiple scales needs to be integrated. Single-unit recordings in rodents suggest that gradients of temporal dynamics in the hippocampus and entorhinal cortex support this integration. In humans, gradients of representation are observed, such that granularity of information represented increases along the long axis of the hippocampus. The neural underpinnings of this gradient in humans, however, are still unknown. Current research is limited by coarse fMRI analysis techniques that obscure the activity of individual voxels, preventing investigation of how moment-to-moment changes in brain signal are organized and how they are related to behavior. Here, we measured the signal stability of single voxels over time to uncover previously unappreciated gradients of temporal dynamics in the hippocampus and entorhinal cortex. Using our novel, single voxel autocorrelation technique, we show for the first time a medial-lateral hippocampal gradient, as well as a continuous autocorrelation gradient along the anterolateral-posteromedial entorhinal extent. Importantly, we show that anterior-posterior and medial-lateral hippocampal autocorrelation gradients were modulated by navigational difficulty, indicating that changes in signal stability are relevant for behavior. Our method and findings open the door for future research on how temporal gradients within these structures support the integration of information for goal-directed behavior.

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Conflict of interest statement

The authors declare no competing financial interests.

Introduction

To enable efficient goal-directed behaviour, information must be represented and integrated across multiple temporal and spatial scales. It has been proposed that neural signal gradients in the hippocampus and entorhinal cortex support such multi-scale representations in rodents, but evidence in humans is sparse and has methodological limitations. Previously, fMRI analysis techniques have uncovered local signal gradients in the human hippocampus (Brunec, Bellana, et al., 2018). These investigations, however, have been limited by analyzing patterns of activity across relatively coarse regions of interest, making it unclear how sustained versus rapidly changing signals are distributed throughout the hippocampus. Many of these analyses use predetermined anterior and posterior anatomical masks, which limit our ability to detect neural signal gradients in an unsupervised way, therefore preventing us from investigating gradients that exist along both anterior-posterior and medial-lateral axes of the hippocampus. Moreover, there have been no prior investigations of autocorrelation gradients in the entorhinal cortex, despite evidence of its role in spatial and temporal representations during navigation. To address these limitations, we have developed a novel, data-driven analysis based on autocorrelation of single voxels in fMRI during rest and navigation. This technique allows us, for the first time, to track the signal stability of individual voxels and their spatial distribution in an unconstrained way along both the anterior-posterior and medial-lateral axes of the hippocampus and entorhinal cortex. Based on this single voxel analysis we uncover gradients of neural signal dynamics along these axes in both structures and relate them to behavior.

In rodents, place fields in the ventral hippocampus (homologous to the anterior hippocampus in humans) span larger areas, show a higher degree of overlap, and higher correlation in their firing across time, compared to the dorsal hippocampus (homologous to the posterior hippocampus in humans) (Hasselmo, 2008; Jung et al., 1994; Kjelstrup et al., 2008; Komorowski et al., 2013). A similar gradient of hippocampal organization is also observed in the human hippocampus. Tracking moment-to-moment similarity across patterns of voxels during virtual navigation, Brunec, Bellana, et al. (2018) found that signal similarity was significantly greater within the anterior hippocampus relative to the posterior hippocampus, indicating that, as in the rodent ventral hippocampus, the human anterior hippocampus demonstrates slower changing signals that are sustained across time and space. These results suggest that a relatively stable pattern of activity in the rodent and human hippocampus follows a scaled gradient, from faster changing signal in the posterior (dorsal) hippocampus to slower changing

signal in the anterior (ventral) hippocampus. This gradient organization might
underlie fine-to-coarse mnemonic representation, particularly when a different
granularity of information needs to be maintained across time (Brunec &
Momennejad, 2019; Robin & Moscovitch, 2017). In addition to the dorsal-ventral
gradient of spatial representation observed in rodents, research suggests a
difference in spatial selectivity along the proximodistal axis (homologous to
medial-lateral in humans), specifically in CA1 (Igarashi et al., 2014), yet whether
a similar medial-lateral distinction exists in the human hippocampus is still
unclear (Hrybouski et al., 2019).
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A key input structure to the hippocampus that has been implicated in integrating
information over time during navigation is the entorhinal cortex. Prior research
has found distinct functional differentiation between the anterolateral and
posterior-medial aspects of the entorhinal cortex (ERC), but there have been no
prior investigations of neural signal gradients in the ERC. The lateral ERC in
rodents, and the homologous anterolateral ERC in humans, supports within-
object and object-location coding, as well as temporal information processing
(Bellmund et al., 2019; Montchal et al., 2019; Olsen et al., 2017; Tsao et al.,
2018; Yeung et al., 2017; 2019). In contrast, the posteromedial ERC in humans,
has been primarily linked to scene processing (Berron et al., 2018; Maass et al.,
2015; Navarro Schröder et al., 2015) and related to grid cell organization
(Bellmund et al., 2016), consistent with evidence of grid cells in the medial ERC
in rodents (Hafting et al., 2005). Given prior evidence of functional distinctions of
the ERC into anterolateral and posteromedial regions, we developed a data-
driven method to investigate directly, a continuous neural signal gradient in both
the anterior-posterior and medial-lateral axes of this structure.
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To understand how a graded organization of signal dynamics in the hippocampus
and ERC supports goal-directed behavior, we developed an analytic approach of
temporal autocorrelation at the single voxel level, which we implemented during
both rest and navigation. Temporal autocorrelation represents the degree of
similarity between a signal and the temporally shifted, or lagged, version of the
signal over successive time intervals (Figure 1A). Conventionally, it is assumed
that this autocorrelation in fMRI data originates from physical and physiological
noise (Arbabshirani et al., 2014; Bollmann et al., 2018; Bullmore et al., 2001;
James et al., 2019; Lenoski et al., 2008; Lund et al., 2006; Purdon & Weisskoff,
1998) or the hemodynamic response function (Arbabshirani et al., 2014; James
et al., 2019; Rajapakse et al., 1998) and, therefore, has been considered
irrelevant to brain function. Recently, however, Arbabshirani et al. (2019) found
that autocorrelation reflects changes in cognitive state (task vs. rest) as well as

changes in mental state (healthy control vs. schizophrenia), suggesting that the
observed changes in the autocorrelation are also modulated by cognitive
processes. Prior studies, however, have been limited and are unable to answer
the question of how temporal autocorrelation is directly related to behavior.
Examining the temporal autocorrelation of single voxels during an active
navigation task, therefore, is important for understanding how a stable, highly
correlated signal is relevant for behavior.
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Investigating the fMRI signal at the single voxel level allows us to measure neural
gradients with more precision than previous methods. While studies with fMRI in
humans suggest that functional heterogeneity exists along the long axis of the
hippocampus (Nadel et al., 2013; Poppenk et al., 2013; see Grady, 2020 for a
review) and medial-lateral extent of the ERC (e.g., Hafting et al., 2005; Maass et
al., 2015; Navarro Schröder et al., 2015), previous analysis techniques have
been limited to investigations using predetermined anatomical masks, which
obscures the contribution of individual voxels, making it unclear whether graded
signals extend along multiple axes in these regions. Furthermore, examining the
autocorrelation at the single voxel level allows for a finer-grained analysis that
may be more sensitive to differences in navigational performance and can help
us to determine how a scaled gradient of signal similarity might be employed to
integrate representations across spatial scales during navigation. We, therefore,
combine our single voxel autocorrelation approach with an unconstrained
clustering method to determine how temporal autocorrelation is distributed in
multiple dimensions throughout the hippocampus and ERC.
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Here we present the first evidence of a medial-lateral neural signal gradient in the
hippocampus as well as a novel continuous gradient in the ERC. Using resting
state fMRI data with high spatial and temporal resolution from the Human
Connectome Project (HCP), we measured single voxel autocorrelation in the
hippocampus and ERC. Specifically, we measured the similarity of single voxels
over time by correlating the timecourse of each voxel with temporally shifted
versions of itself (Figure 1A). We applied data-driven clustering to determine how
temporal autocorrelation was spatially distributed throughout the hippocampus
and ERC. We found high autocorrelation in the anterior-medial hippocampus and
posteromedial ERC and low autocorrelation in the posterior-lateral hippocampus
and anterolateral ERC. Using task-based fMRI, we replicated these results and
also demonstrated that increases in navigation difficulty were associated with
increases in autocorrelation in the anterior-medial hippocampus. Our single voxel
autocorrelation approach yields consistent and precise gradients of single voxel
autocorrelation in the hippocampus and ERC, providing a powerful new

continuous and data-driven method that can illuminate how temporal dynamics in
brain signals relate to complex cognition.
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124 **Results**
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Dataset 1: Resting state fMRI
Hippocampus
Spatial distribution of single voxel autocorrelation
To examine hippocampal dynamics at the single voxel level when no cognitive
demands were placed on participants, we first analyzed resting-state fMRI data
from 44 participants from the Human Connectome Project (HCP) Retest dataset
(2 runs per participant). Here, we correlated the timecourse of activity of each
voxel in the hippocampus with activity in that same voxel shifted by a temporal
lag of 1 TR (Dataset 1 TR = 720 ms). We repeated this process until a maximum
temporal shift of 4 seconds was reached, or 5 lags (Figure 1A). A map of single
voxel autocorrelation values throughout the hippocampus was generated for
each lag separately (for a theoretical schematic, see Figure 1B).
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We found that single voxel autocorrelation maps at the group level (lags 1-5)
showed a notable difference in the distribution of single voxel autocorrelation
values along the hippocampal axis (Figure 2A). More specifically, voxels with
higher single voxel autocorrelation were mainly in the anterior-medial region
whereas voxels with lower single voxel autocorrelation were mainly in the
posterior-lateral region (in both left and right hippocampus). As shown in Figure
2A, although the overall autocorrelation decreased as the lag increased, the
overall pattern of autocorrelation gradients was similar for lags 1-5.
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Single voxel autocorrelation – Reliability results
We next tested the reliability of these results. Here we defined a reliable result as
one in which single voxel autocorrelation vectors generated from two runs of the
same participant were more similar than two runs from *different* participants
(lower intra-subject Euclidean distances compared to inter-subject Euclidean
distances). Nonparametric permutation tests comparing intra-subject and inter-
subject Euclidean distance revealed reliable results in both the left (intra-subject:
7.43 ± 2.07, inter-subject: 9.38 ± 2.22, $P < 0.0001$) and right hippocampus (intra-
subject: 7.22 ± 1.98, inter-subject: 9.02 ± 2.02, $P < 0.0001$) (Figure 3A). These
high intra-subject similarity values suggest that the single voxel autocorrelation
pattern is an intrinsic feature of the brain, likely originating from neuronal
sources, rather than noise or imaging artifacts.
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Figure 1. A) Method. For each voxel, the timecourse of activity was successively
temporally shifted by 1 TR and correlated with itself. This was repeated for a total shift of
4 seconds (i.e., 5 lags for resting state data (Dataset 1) and 2 lags for navigation data
(Dataset 2)). This resulted in a vector of single voxel autocorrelation values, with each
value corresponding to a different lagged correlation. **B) Single voxel autocorrelation**
(hypothetical values). The procedure was repeated for all voxels in an ROI. To
examine the spatial distribution of the single voxel autocorrelation, we plot the group-
level single voxel autocorrelation maps for each lag, averaged across runs and
participants. **C) Autocorrelation clustering (hypothetical values).** The autocorrelation
values for each lag were stored in a vector (single voxel autocorrelation vector). The
voxels in the ROI were clustered based on the similarity (Euclidean distance) of single
voxel autocorrelation vectors. Single voxel autocorrelation vectors were clustered
according to their Euclidean distance (Blondel et al., 2008). Clustering was performed at
the individual-level and at the group-level.

Autocorrelation Clustering

We applied a Louvain clustering method using modularity maximization without predefining the number of clusters (Blondel et al., 2008) to the group-level single voxel autocorrelation vectors (for a theoretical schematic, see Figure 1C). This data-driven clustering approach revealed three distinct clusters in both the left and right hippocampus (Figure 2B); notably, past work that segmented the hippocampus into two ROIs (anterior and posterior) a priori would not have been able to detect the presence of this third cluster. Consistently across all 5 lags we found that Cluster 1 had the highest single voxel autocorrelation values and was located in the anterior-medial hippocampus (Figure 2D). Cluster 3 had the lowest single voxel autocorrelation values and was located in the posterior-lateral part of the hippocampus. Cluster 2 had intermediate single voxel autocorrelation values and was located between Clusters 1 and 3. These three clusters were also reliably observed at the individual level (cluster maps from two runs of an example participant are shown in Figure 2B).

In summary, clustering revealed a high-to-low single voxel autocorrelation gradient along the anterior-posterior axis, consistent with what has been previously found in the literature (Brunec, Bellana, et al., 2018; Raut et al., 2020). In addition, we found differences along the medial-lateral axis, as well as a prominent anterior-medial cluster of high single voxel autocorrelation that could be distinguished from a posterior-lateral cluster of low single voxel autocorrelation. While previous methods using predetermined anterior/posterior ROI masks might have missed this medial-lateral distinction, our data-driven method provides evidence that an autocorrelation gradient exists along multiple spatial dimensions.

Autocorrelation Clustering – Reliability results

The reliability of single voxel autocorrelation clustering was evaluated by measuring spatial overlap between clusters, calculated by the Jaccard coefficient (Figure 3B). Here we defined a reliable result as one in which the spatial distribution of autocorrelation clusters was consistent across the two runs of the same participant, indicated by greater overlap (higher Jaccard coefficient) among clusters *within* an individual compared to *between* different individuals. Using nonparametric permutation, we found high reliability for clusters in the bilateral hippocampus, specifically Cluster 1 (Left: $P < 0.001$; Right: $P < 0.001$) and Cluster 3 (Left: $P < 0.001$; Right: $P < 0.001$). These findings of high intra- and inter-subject overlap suggest that Clusters 1 and 3 were highly reliable, within individuals. Cluster 2, however, had significantly lower overlap (Left: $P = 0.06$; Right: $P = 0.007$), suggesting more variability within individuals.

Gradients of single voxel autocorrelation (lag 1)

The single voxel autocorrelation and autocorrelation clustering results presented above both suggest the presence of an autocorrelation gradient along two main axes: the anterior-posterior axis and the medial-lateral axis. To more precisely examine these individual gradients, we plotted the single voxel autocorrelation across hippocampal slices along the X (medial-lateral), Y (posterior-anterior), and Z (inferior-superior) axes. We observed consistent gradients in every participant. Specifically, single voxel autocorrelation gradually decreased in the medial-to lateral direction and increased in the posterior-to-anterior direction (Figure 2C; we focused on lag 1, but a similar pattern was revealed across all lags, as shown in Figure 2A). A rough gradient of high-to-low autocorrelation was also observed in the inferior-superior axis, which is due to the angle of the hippocampus (i.e., the anterior hippocampus is located more inferiorly relative to the posterior hippocampus). When we investigated the spatial distribution of the three clusters (projected on the background of the plots in Figure 2C), we observed a gradient of cluster assignment that complemented the single voxel autocorrelation gradients. Specifically, high-to-low single voxel autocorrelation gradients were also associated with a cluster gradient from Cluster 1 to Cluster 3.

Figure 2. Hippocampus. Single Voxel Autocorrelation. A) Group-level single voxel
autocorrelation maps averaged across all runs for all participants. **Autocorrelation**
Clustering. B) Group-level clusters (top) and run-level cluster maps for two runs from an
example participant (bottom). Three distinct clusters were found at both the group and
the individual run-level. Cluster 1 was located in the anterior-medial hippocampus,
Cluster 3 was located in the posterior-lateral hippocampus, and Cluster 2 was located
between Cluster 1 and 3. **C) Single Voxel Autocorrelation: Lag 1.** Single voxel
autocorrelation (lag 1) averaged per slice and projected into three axes (X, Y, and Z) to
visualize changes in medial-lateral, anterior-posterior, and inferior-superior directions
(plots depict left hemisphere; right hemisphere looked similar). The average cluster
assignment of voxels on each slice is presented as the background color to show the
gradation in values along the three axes. **D) Average Cluster Value Across Lag.**
Average group-level single voxel autocorrelation values for each cluster at each lag.
Cluster 1 was associated with the highest single voxel autocorrelation values, Cluster 2
with intermediate values, and Cluster 3 with the lowest. This was consistent across all 5
lags.
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Figure 3. Hippocampal and Entorhinal cortex reliability measures. A,C) Single Voxel Autocorrelation Reliability. Distribution of shuffled and permuted mean difference of intra- and inter-subject Euclidean distances for the (A) hippocampus and (C) entorhinal cortex. Dashed lines represent the observed mean difference between intra- and inter-subject Euclidean distance. Significant negative values indicate that single voxel autocorrelation values were more similar within an individual than across individuals. **B, D) Autocorrelation Cluster Reliability.** Distribution of shuffled and permuted mean difference of intra- and inter-subject Jaccard coefficients for each cluster. Dashed lines represent the observed difference between intra- and inter-subject Jaccard coefficients for each cluster. (B) In both hemispheres of the hippocampus, Clusters 1 and 3 were more reliable within individuals compared to Cluster 2. (D) In the entorhinal cortex, Cluster 1 and Cluster 2 were reliable within individuals in the left hemisphere, whereas Cluster 1 and 3 were reliable within individuals in the right hemisphere.

Entorhinal cortex
Spatial distribution of single voxel autocorrelation
We repeated the analyses above in the ERC. To illustrate the distribution of
autocorrelation values of individual voxels throughout the ERC, we plotted the
group-level single voxel autocorrelation maps for lags 1-5 (Figure 4A). The maps
illustrate a difference in single voxel autocorrelation throughout the ERC.
Specifically, voxels with higher single voxel autocorrelation were mainly in the
posterior-medial region whereas voxels with lower single voxel autocorrelation
were mainly in the anterior-lateral region (in both left and right ERC).
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Single voxel autocorrelation – Reliability results
Nonparametric permutation tests comparing intra-subject and inter-subject
Euclidean distance revealed reliable results in both the left (intra-subject: 11.43 ±
3.64, inter-subject: 12.87 ± 2.83, $P < 0.001$ and right ERC (intra-subject: 10.41 ±
2.63, inter-subject: 13.19 ± 2.53, $P < 0.001$; Figure 3C). This analysis
demonstrates the reliability of the single voxel autocorrelation and suggests that
single voxel autocorrelation patterns between vectors generated from two runs of
the *same* participant were more similar than two runs from *different* participants
(lower intra-subject Euclidean distances compared to inter-subject Euclidean
distances).
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Autocorrelation Clustering
The group-level clustering analysis on the voxels within the ERC revealed two
distinct clusters in the left hemisphere and three clusters in the right (Figure 4B).
For comparison, cluster maps from two runs of an example participant are shown
in Figure 4B. Cluster 1 was located in the posteromedial ERC and had the
highest single voxel autocorrelation values in both left and right hemispheres.
Cluster 2 was observed in the left hemisphere and was located towards the
anterior-lateral ERC with low single voxel autocorrelation values. In the right
hemisphere it was an intermediate cluster. Cluster 3 was only observed
consistently in the right hemisphere and was located in the anterior-lateral ERC
with the lowest single voxel autocorrelation values. We computed the group-level
single voxel autocorrelation for each cluster and plotted it across all 5 lags
(Figure 4D). Across all 5 lags, Cluster 1 consistently had the highest single voxel
autocorrelation values, followed by Cluster 2 and Cluster 3.
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Autocorrelation Clustering – Reliability results
The reliability measure for ERC clusters was calculated by the Jaccard
coefficient (Figure 3D). Nonparametric permutation tests comparing intra-subject
and inter-subject cluster overlap revealed reliable results in the left and right

hemisphere. In the left hemisphere, the Cluster 1 (P < 0.001) and Cluster 2 (P <
0.001) were reliable. In the right hemisphere, Cluster 1 (P < 0.001) and Cluster 3
(P < 0.001) were reliable. This suggests that these clusters were highly reliable
within individuals. In the right hemisphere, Cluster 2 had very small Jaccard
values, suggesting less reliability within individuals (Right: P = 0.53).
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Gradients of single voxel autocorrelation (lag 1)
Single voxel autocorrelation values for lag 1 were projected onto X (medial-
lateral), Y (posterior-anterior), and Z (inferior-superior) axes. As shown in Figure
4C, in every participant, single voxel autocorrelation values gradually decreased
in the medial-to-lateral direction and the posterior-to-anterior direction (Figure
4C). We found a gradient of low-to-high autocorrelation along the inferior-
superior axis, which is due to the fact that the posterior region of the ERC is more
superior than its anterior region. We observed a gradient of cluster assignment
that complemented the single voxel autocorrelation gradients, where high-to-low
gradients were also associated with a cluster gradient from Cluster1 to Cluster 2.
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Entorhinal Cortex

Figure 4. Entorhinal cortex. Single Voxel Autocorrelation. A) Group-level single voxel autocorrelation maps averaged across all runs for all participants. **Autocorrelation Clustering. B)** Group-level clusters (top) and run-level cluster maps for two runs from an example participant (bottom). Two distinct clusters were found in the left hemisphere and three in the right hemisphere. In the left hemisphere, Cluster 1 was located in the posterior-medial ERC and Cluster 2 was in the anterior-lateral ERC. In the right hemisphere Cluster 1 was located in the posterior-medial ERC, Cluster 3 was located in the anterior-lateral ERC, and Cluster 2 was located between Cluster 1 and 3. **C) Single Voxel Autocorrelation: Lag 1.** Single voxel autocorrelation projected below onto three axes (X, Y, and Z) to visualize changes in medial-lateral, anterior-posterior, and inferior-superior directions (for the left hemisphere; right hemisphere looked similar). The average cluster assignment of voxels on each slice is presented as the background color to show the gradation in values along the three axes (Note the gradation depicts only Cluster 1 and 2 as there were only two significant clusters found in the left hemisphere). **D) Average Cluster Value Across Lag.** Average group-level single voxel autocorrelation values for each cluster at each lag. In the left hemisphere, Cluster 1 was associated with the highest single voxel autocorrelation values and Cluster 2 with low autocorrelation values. In the right hemisphere, Cluster 1 was associated with the

highest single voxel autocorrelation, Cluster 2 with intermediate values, and Cluster 3

with the lowest. This was consistent across all 5 lags.

Dataset 2: Navigation *fMRI*

We next aimed to replicate the observed effects in task fMRI and relate changes

in single voxel autocorrelation to behavior. Specifically, we were interested in

how single voxel autocorrelation throughout the hippocampal long axis might be

modulated by differences in difficulty during a temporally-extended navigation

task. Therefore, we performed our single voxel autocorrelation analyses on a

task fMRI dataset acquired while participants navigated in a familiar virtual reality

environment (previously described in Brunec, Bellana et al., 2018). Here, 19

participants were scanned while navigating Google Street View routes around

the city of Toronto. Participants navigated four different types of routes that

varied in their navigational difficulty: GPS (unfamiliar routes guided by an arrow),

Familiar (highly familiar routes), Unfamiliar (routes that were less familiar), and

Mirrored (familiar routes that were left-right reversed). Participants completed

four unique routes in each condition, sixteen routes in total (1 route = 1 scanned

run). Due to the lower spatial resolution in this dataset we were not able to

examine the ERC and, thus, these analyses focused only on the hippocampus.

Hippocampus

Spatial distribution of single voxel autocorrelation

To compute the single voxel autocorrelation, we completed the same procedure

outlined in Dataset 1. In Dataset 2 the TR was 2000 ms; therefore, single voxel

autocorrelation for 2 lags (or 2 TRs) was calculated. We observed a difference in

single voxel autocorrelation along the anterior-posterior and medial-lateral

hippocampal axes, where voxels with higher single voxel autocorrelation were

found in the anterior-medial hippocampus and voxels with lower single voxel

autocorrelation were found in the posterior-lateral hippocampus. Figure 5A

shows the group-level single voxel autocorrelation maps for the four navigation

conditions (as single voxel autocorrelation maps for lags 1-2 were similar, only

lag 1 is depicted in Figure 5A). The spatial distribution of single voxel

autocorrelation was similar across navigation conditions and was also similar to

the findings from Dataset 1. In the next section, we investigate the differences

between conditions in more depth.

Figure 5. A) Single Voxel Autocorrelation: Lag 1. Single voxel autocorrelation values
at lag 1 for every voxel in the hippocampus during spatial navigation. These values are
averaged across run and participant for each of the GPS, Familiar, Unfamiliar and
Mirrored conditions. A gradient from high to low autocorrelation is observed in the
anterior-posterior and medial-lateral axes, across all navigation conditions. **B)**
Autocorrelation Clustering. Cluster maps averaged across run and participant for each
route type. High single voxel autocorrelation voxels cluster in the anterior-medial
hippocampus and low single voxel autocorrelation voxels cluster in the posterior-lateral
hippocampus.

Autocorrelation Clustering
In order to determine clusters of single voxel autocorrelation within each
navigational condition, we repeated the autocorrelation clustering procedure
described above in Dataset 1 within the hippocampus. As with Dataset 1, this
revealed three distinct clusters in the left and right hemispheres for the Familiar,
Unfamiliar and Mirrored conditions (Figure 5B). For Familiar, Unfamiliar, and
Mirrored conditions, Cluster 1 was located in the anterior-medial HPC and had
the highest single voxel autocorrelation. Cluster 3 was located in the posterior-
lateral hippocampus and had the lowest single voxel autocorrelation. Cluster 2
was located between Cluster 1 and 3 and had intermediate single voxel
autocorrelation. The GPS condition had three clusters in the right hemisphere
and only two in the left.

Relating single voxel autocorrelation to navigation condition
Subjective difficulty ratings collected after each route (1 = difficult, 9 = easy)
suggested that across the navigation conditions, navigational difficulty increased.
Participants rated the GPS routes as the easiest (M = 7.2, SD = 1.46), followed

415 by the Familiar condition (M = 6.98, SD = 2.05), Unfamiliar condition (M = 4.35,
416 SD = 2.66), and the Mirrored condition, which was subjectively the most difficult
417 (M = 3.97, SD = 2.42).
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As navigation becomes more difficult, it is beneficial to integrate or maintain
information over time, which may be reflected in changes in single voxel
autocorrelation. Specifically, more stable neural dynamics might enable
individuals to maintain information as one moves towards a goal. This prediction
leads to two possibilities. In the first, as navigational difficulty increases we might
observe a uniform change in single voxel autocorrelation across all voxels in the
hippocampus. A second possibility is that as difficulty increases, voxels that tend
to exhibit high autocorrelation during rest would differentially increase their
autocorrelation relative to voxels that tend to exhibit low autocorrelation. To
investigate these possibilities, we calculated the slope of the single voxel
autocorrelation (lag 1) along the anterior-posterior and medial-lateral axes. If
navigational difficulty leads to a uniform increase in autocorrelation, we would
observe no changes in the slope across these axes. However, if navigational
difficulty disproportionately affects the regions of the hippocampus that show high
autocorrelation during rest (Figure 2), then more difficult routes would elicit a
larger difference in autocorrelation values along the anterior-posterior and
medial-lateral axes, and therefore, a steeper slope. For easier routes, there
would be less difference in autocorrelation along the two axes, suggesting more
homogeneity of temporal dynamics along the axis and a shallower slope of
autocorrelation.
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Anterior-posterior HPC axis
Comparing single voxel autocorrelation slopes
We compared autocorrelation slopes in the four route conditions: GPS, Familiar,
Unfamiliar, and Mirrored. For each participant, we averaged the single voxel
autocorrelation (lag 1) across all voxels on each 3mm slice of the hippocampus
(posterior-to-anterior direction) and calculated the slope coefficient across slices.
In both the left and right hemisphere, across all four navigation conditions, the
slope was positive, suggesting lower autocorrelation in the posterior
hippocampus and higher autocorrelation in the anterior hippocampus, which is
consistent with our findings from the clustering and single voxel autocorrelation
lag 1 analyses. Across participants, Mirrored runs had steepest slopes (*Left:* M =
0.79, SD = 0.60; *Right:* M = 0.55, SD = 0.80) followed by Unfamiliar (*Left:* M =
0.69, SD = 0.53; *Right:* M = 0.41, SD =0.40), Familiar (*Left:* M = 0.63, SD = 0.46;
Right: M = 0.31, SD = 0.25), and GPS routes (*Left:* M = 0.53, SD = 0.42; *Right:* M
= 0.21, SD = 0.28).

To test whether there was a significant difference between single voxel
autocorrelation during different navigation conditions, we ran a mixed effects
model on the single voxel autocorrelation slopes along the anterior-posterior axis.
We included hemisphere and condition (GPS, Familiar, Unfamiliar, and Mirrored)
as predictors in the model and participants as a random intercept in the random
effects term. We found a significant effect of hemisphere ($F(1, 481.99) = 42.22$, p
$< .001$) and a significant effect of navigation condition ($F(3, 483.04) = 6.92$, $p <$
$.001$) (Figure 6A). Their interaction was not significant.

A post hoc analysis of the main effect of hemisphere revealed that the single
voxel autocorrelation slope was greater in the left hippocampus compared to the
right hippocampus ($t(482) = 6.49$, $p < .001$). Pairwise comparisons of the different
navigational conditions (collapsed across hemisphere) revealed that single voxel
autocorrelation slopes were significantly greater for the Mirrored compared to
GPS ($t(484) = 3.88$, $p < .001$) and Familiar ($t(482) = 3.71$, $p < .01$). There was no
significant difference between Mirrored and Unfamiliar conditions. These results
suggest that, across hemispheres, the single voxel autocorrelation slopes along
the anterior-posterior axis were modulated by navigation difficulty: navigation
runs with a steeper gradient of autocorrelation were related to more difficult
navigation conditions. We compared the average single voxel autocorrelation at
the two posterior-most and two anterior-most slices and found that single voxel
autocorrelation was higher in the anterior hippocampus compared to the
posterior hippocampus in both the left and right hemisphere (Left: anterior >
posterior $t(1998) = 22.23$, $p < .001$; Right: anterior > posterior $t(1998) = 13.49$, p
$< .001$). This finding suggests that increases in the autocorrelation slope along
the anterior-posterior axis across conditions were driven by an increase in the
anterior hippocampus.

Figure 5. Effect of navigational condition on single voxel autocorrelation slopes.
Average single voxel autocorrelation per slice along the anterior-posterior and medial-
lateral axes for each navigation condition. **A) Anterior-posterior axis.** The left
hippocampus had greater single voxel autocorrelation slopes compared to the right
hippocampus. Across both hemispheres, slope along the anterior-posterior axis was
modulated by navigational condition. The slope was greatest when participants
navigated difficult routes (Mirrored and Unfamiliar routes) compared to easy routes (GPS
and Familiar routes) **B) Medial-lateral axis.** The left hippocampus had greater single
voxel autocorrelation slopes compared to the right hippocampus. Across both
hemispheres, slope along the medial-lateral axis was modulated by navigational
condition. The slope was greatest when participants navigated Mirrored routes
compared to GPS, Familiar, and Unfamiliar routes. Bold lines represent the group
average across all participants, faded lines represent each participant.
498
Medial-lateral HPC axis
Comparing single voxel autocorrelation slopes
For each participant, we averaged the single voxel autocorrelation (lag 1) across
all voxels on each 3mm slice of the hippocampus (lateral-to-medial direction) and
calculated the slope coefficient across slices. In both the left and right
hemisphere, across all four navigation conditions, the slope was positive,
suggesting lower autocorrelation in the lateral hippocampus and higher
autocorrelation in the medial hippocampus. This observation is consistent with
our findings from the clustering and single voxel autocorrelation lag 1 analyses.
Across participants, Mirrored runs had steepest slopes (*Left:* M = 1.63, SD =
1.15; *Right:* M =1.45, SD = 1.77) followed by Unfamiliar (*Left:* M = 1.37, SD =

0.95; *Right:* M = 1.13, SD = 1.20), Familiar (*Left:* M = 1.21, SD = 0.74; *Right*: M =
0.92, SD = 0.98), and GPS routes (*Left:* M =1.08, SD = 0.80; *Right:* M = 0.89, SD
= 1.45).

We ran a mixed effects model on the single voxel autocorrelation slopes along
the medial-lateral axis with hemisphere and condition as predictors and
participant as a random intercept in the random effects term. We found a
significant effect of hemisphere ($F(1, 482.03) = 5.03$, $p < .05$) and a significant
effect of navigation condition ($F(3, 482.71) = 7.10$, $p < .001$) (Figure 6B). Their
interaction was not significant.

A post hoc analysis of the main effect of hemisphere revealed that the single
voxel autocorrelation slopes were greater in the left than the right hippocampus
($t(482) = 2.24$, $p < 0.05$). Pairwise comparisons of the different navigational
conditions (collapsed across hemisphere) revealed that single voxel
autocorrelation slopes were significantly greater for the Mirrored compared to
GPS ($t(483) = 3.42$, $p < .01$), greater for Mirrored compared to Familiar ($t(482) =$
4.18, $p < .001$), and greater for Mirrored compared to Unfamiliar ($t(482) = 2.61$, p
$< .05$). These results suggest that, across hemispheres, the single voxel
autocorrelation slopes along the medial-lateral axis were modulated by
navigation difficulty: navigation runs that had a steeper gradient of
autocorrelation were related to more difficult navigation conditions. We compared
the average single voxel autocorrelation at the two medial-most and two lateral-
most slices and found that single voxel autocorrelation was higher in the medial
hippocampus than the lateral hippocampus in both the left and right hemisphere
(Left: medial > lateral $t(1998) = 17.76$, $p < .001$; Right: medial > lateral $t(1998) =$
14.91, $p < .001$). This suggests that increases in the autocorrelation slope along
the medial-lateral axis across conditions is driven by an increase in the medial
hippocampus.

Discussion

Here we present a novel autocorrelation measure to investigate intra-
hippocampal and intra-entorhinal processing. We provide the first evidence of a
medial-lateral gradient of autocorrelation in the hippocampus, as well as a
posterior-medial and anterior-lateral gradient in the ERC. We found that voxels in
the anterior-medial hippocampus have a highly correlated, slower changing
signal, whereas voxels in the posterior-lateral hippocampus have a less
correlated, faster changing signal (Figure 2) (Brunec, Bellana, et al., 2018; Raut
et al., 2020). Our study highlights the importance of examining the medial-lateral

axis of the hippocampus, which has previously been an under-studied feature of
hippocampal organization. We find novel evidence for a continuous gradient in
the ERC, with greater autocorrelation in the posteromedial ERC and lower
autocorrelation in the anterolateral ERC (Figure 4). Lastly, the present study is
the first to show that gradients of single voxel autocorrelation in the hippocampus
are related to behavior during navigation. Specifically, autocorrelation gradients
in the anterior-posterior and medial-lateral axes, as measured by the slope,
increased for difficult routes and were steepest in the left hemisphere (Figure 6).
This increase in slope was driven by increases in the anterior-medial
hippocampus.
560
Our data-driven approach — which allows voxels to cluster according to their
single voxel autocorrelation, uncovered a multidimensional gradient in both the
anterior-posterior and medial-lateral axes in both the hippocampus and ERC
(Figure 2 & 4). In the hippocampus, the anterior-posterior axis has been studied
with respect to its role in representing graded information, for example coarse-
grained to fine-grained information (Poppenk et al. 2013; Strange et al., 2014),
large to small spatial distances (Evensmoen et al., 2013; Nielson et al., 2015;
Peer et al., 2019;) and long to short temporal distance (Bellmund et al., 2019;
Nielson et al., 2015). Investigations of representational differences along the
medial-lateral axis, however, have been limited because prior work has used
predefined anatomical segmentations limited to the anterior and posterior
portions of the long axis of the hippocampus. Our single voxel autocorrelation
method is not restricted by predefined ROIs and proves to be a more precise
measure that detects subtle differences in signal along the medial-lateral axis
that have been previously overlooked and that are modulated by navigational
difficulty. In addition to the hippocampus, we found similar distinctions in the
ERC. We observed a gradient of single voxel autocorrelation organization, such
that greater single voxel autocorrelation was observed in the posterior-medial
region and lower single voxel autocorrelation in the anterolateral region of the
ERC (Figure 4). This gradient is consistent with previous neuroimaging
investigations of ERC which used high-resolution fMRI and functional
connectivity to define distinct subregions within the human ERC (Maass et al.,
2015; Navarro Schröder et al., 2015). Our analytic technique, however, goes
beyond this prior work by demonstrating, for the first time, continuous gradients
of autocorrelation in the ERC.
586
The present study demonstrates that the autocorrelation of the fMRI signal is not
just global noise, but instead carries meaningful information about brain function
that is directly related to behavior. Autocorrelation is frequently characterized as

noise that masks meaningful signals and is unrelated to cognition, but recent
research suggests that autocorrelation might be a global organizing principle and
reflects intrinsic functional hierarchies in the brain (Irish & Vatansever, 2020;
Raut et al., 2020). For example, an analysis of resting state fMRI data calculated
the autocorrelation decay in single voxels across a temporal window (0-8
seconds) and found a significant large-to-small timescale gradient along the
anterior-posterior axis in the hippocampus (Raut et al., 2020), which is consistent
with reports by Brunec, Bellana, et al. (2018). Recent research has also linked
autocorrelation with global differences in cognitive state (task vs. rest) and
mental state (healthy vs. schizophrenia) (Arbabshirani et al., 2019). While this
study cannot address the direct link between the autocorrelation gradients and
behavior, this work suggests that autocorrelation can be used to discriminate
between cognitive states that are uniform across the brain, leaving open the
question of how autocorrelation gradients in specific brain regions might be
related to differences in cognition during a behavioral task. Our analysis
technique demonstrated novel gradients during resting state, and can also be
applied to task related activation to reveal their relation to on-going behavior and
is the first to show that changes in single voxel autocorrelation gradients are
directly related to changes in difficulty during a navigation task.
609
Anterior hippocampal voxels are more stable across time compared to the
posterior hippocampus, which might enable the anterior hippocampus to maintain
prior information across time during goal-directed navigation (Brunec, Bellana, et
al., 2018). Our method proved to be a more sensitive measure than previous
techniques (e.g., Brunec, Bellana et al., 2018) because we were able to show
differences in autocorrelation across navigation conditions. More specifically we
found that the autocorrelation in the anterior-medial hippocampus increased
during navigation of difficult routes (Figure 6). The autocorrelation signal may
reflect the mechanism by which the hippocampus holds onto the past and carries
it forward during navigation when we are in unfamiliar or unpredictable
environments. For example, when navigating an unfamiliar route to a distant
goal, the local details of the environment might not be helpful to orient oneself in
relation to the goal; it may be more efficient, therefore, to keep in mind a coarser,
overall map of the environment with information about steps already taken in
order to reach the goal destination successfully. This large-scale representation
may not be as useful to keep online during navigation of well-known or familiar
routes where local details are sufficient for orienting and navigating to the goal,
which could explain the decreased single voxel autocorrelation in the signal
throughout the familiar routes (Figure 6). This hypothesis is supported by
previous research which has shown that the anterior hippocampus plays an

important role in representing larger spatial and temporal distances (Evensmoen
et al., 2013; Nielson et al., 2015) as well as representing coarser-grained, global
representations (Collin et al., 2015).
633
We found that both of the single voxel autocorrelation gradients (anterior-
posterior and medial-lateral) were steeper in the left hemisphere compared to the
right. It is still unclear whether this is representative of a stable difference in
autocorrelation between the hemispheres or whether this reflects different types
of information that are engaged across the two hemispheres during navigation.
Future research is needed to determine the nature of this hemispheric difference.
640
Another non-mutually exclusive possibility is that the single voxel autocorrelation
is representative of predictions that are cast into the future. The notion that
increased temporal similarity is indicative of an extended spatiotemporal
representation is supported by recent work investigating the predictive horizons
along the hippocampal anteroposterior axis during navigation (Bruenc &
Momennejad, 2019). Brunec and Momennejad (2019) found that as participants
virtually navigated familiar, real-world routes (a subset of the familiar routes
presented here), hippocampal activity was related to a hierarchical scale of
horizon representations, in which the posterior hippocampus represented steps
closer in the future trajectory (~25m) while the anterior hippocampus represented
steps further in the future trajectory (~175m). It is possible, therefore, that the
single voxel autocorrelation we observed helps represent an upcoming
navigational trajectory, with immediate goals represented in posterior-lateral
regions and more distal goals in the anterior-medial hippocampus. The predictive
role of the hippocampus has also been observed in perception, particularly when
the stimulus was visually complex (Kok et al., 2020). Our method and findings
open the door for future studies using high resolution neuroimaging in
combination with a task that parametrically modulates the amount of information
that is carried over time in both predictable (familiar) and unpredictable
(unfamiliar) environments to uncover content that is carried forward via the
autocorrelation signal.
662
Although we were not able to relate the autocorrelation in ERC to behavior due to
the resolution of the navigation data, if we apply the same logic we used for the
hippocampus, our findings are consistent with the notion that alERC codes for
local details and perceptual aspects of experience, whereas the pmERC codes
for global contexts. Specifically, the (antero-)lateral ERC has been linked to fine-
grained temporal processing (Montchal et al., 2019; Tsao et al., 2018) and to
processing of object-context and within-object details (Yeung et al., 2017; 2019).

The low autocorrelation we observed in the alERC might indicate faster updating
of moment-to-moment changes and therefore support fine-grained
representations. Future investigations can use our method to analyze continuous
changes along both anterior-posterior and medial-lateral axes of the ERC without
being restricted to anatomical subfield segmentations, perhaps revealing a more
nuanced understanding of the organization of the ERC. We observed two
consistent clusters in the left hemisphere and three consistent clusters in the
right hemisphere, which suggests that in this dataset there was more variability in
the left ERC intermediate cluster. Future research is needed to determine
whether this is a stable property of the temporal organization of the left ERC that
can be replicated across other datasets.
681
It is currently unclear how the posterior-medial and anterior-lateral subregions of
the ERC are functionally related to the anterior and posterior regions of the
hippocampus. In the present study we found that clusters in the anterior-medial
hippocampus and posterior-medial ERC had high single voxel autocorrelation,
whereas clusters in the posterior-lateral hippocampus and antero-lateral ERC
had low single voxel autocorrelation. These distinctions along the anterior-
posterior and medial-lateral axes of the ERC are consistent with previous
functional connectivity findings (Navarro Schröder et al., 2015), however
functional connectivity and neuroanatomical studies in humans have been limited
and do not find any clear differences between the anterior and posterior portions
of the hippocampus with respect to their connectivity to different subregions in
the ERC (Maass et al., 2015; Navarro Schröder et al., 2015). Functional
connections between these regions might be evident in the scale of information
processing in the hippocampus and ERC. For example, it is possible that the
pattern of low single voxel autocorrelation in anterior-lateral ERC and posterior-
lateral hippocampus supports fine-grained processing — precise temporal
processing in the anterior-lateral ERC (Bellmund et al., 2019; Montchal et al.,
2019) and local spatial details in the posterior hippocampus (Doeller et al., 2008;
Evensmoen et al., 2013; Hirshhorn et al. 2012; Lee et al., 2012).
701
There are currently no clear neuroanatomical links between the anterior-lateral
ERC and posterior-lateral hippocampus or the anterior-medial hippocampus and
posterior-medial ERC. There are, however, probable connections between the
anterior ERC and lateral hippocampus and posterior ERC with medial
hippocampus (Strange et al., 2014; Witter & Amaral 2020; Nilssen et al., 2019;
Witter et al., 2017). Our results, therefore, open the door for future investigations
to characterize more fully the nature of anterior and posterior hippocampal signal
dynamics in relation to the entorhinal subregions in humans and in relation to

other structures, such as prefrontal cortex (Barredo et al., 2015; Vaidya & Badre,
2020).
712
The results presented here reveal, for the first time, two continuous gradients
along the anterior-posterior and medial-lateral axes in the hippocampus and
ERC. One outstanding question is whether there is new information that can be
gained by investigating the two autocorrelation gradients separately, or whether
the information they represent is redundant. For example, do tasks that evoke a
steep autocorrelation gradient along the anterior-posterior axis necessarily evoke
a similarly steep gradient along the medial-lateral axis or are there tasks in which
these two gradients act in opposing directions (e.g., change in anterior-posterior
slope but no change or change in opposite direction in medial-lateral slope).
Another outstanding question is whether our novel single voxel autocorrelation
method can be applied with shorter timescales so that they can be used with
event-related designs. Here we use the entire timecourse of the voxel's activity to
calculate the single voxel autocorrelation throughout the entire run, but it remains
to be seen whether we can adapt our method to examine how autocorrelation
changes over shorter time windows. This would allow us to ask new questions
about what kind of information is being carried in the autocorrelation signal during
discrete or shorter events and at event boundaries, which are known to trigger
changes in hippocampal activity associated with integration of information across
events (Dubrow & Davachi, 2013; Ezzyat & Davachi, 2014). Finally, this method
can be used to investigate differences in autocorrelation within subfields of the
hippocampus. For example, it has been proposed that CA1 is implicated in
integrating information in memory, whereas DG/CA3 which mediates pattern
separation may be more implicated in making fine distinctions in memory (Kyle et
al., 2015; Leutgeb et al., 2004; Schapiro et al., 2017; Yassa & Stark, 2011).
Integration processes in CA1, therefore, might be supported by voxels with high
single voxel autocorrelation while separation processes in DG/CA3 might be
better supported by low single voxel autocorrelation. Future research using our
method and high-resolution fMRI is needed to test these differences within
subfields.
742
Our studies were inspired initially by single-unit recording studies in rodents
(Brun et al., 2008; Cavanagh et al., 2016; Gothard et al.,1996; Kjelstrup et al.,
2008; Maurer et al., 2005). We believe our findings, however, have gone beyond
replicating the rodent findings in humans, a worthy task in its own right, but
extended the findings to the point that they can now be used to inform future
studies in rodents and humans. We provide some examples in which this is the
case. For example, our method enabled us to find differences in autocorrelation

along the anterior-posterior and medial-lateral axes in the entorhinal cortex,
which have only been examined in a restricted region in rodents (Brun et al.,
2008). Our findings are consistent with neuroanatomical and neurophysiological
divisions in that structure (human: Maass et al., 2015; monkey: Witter & Amaral,
2021; rat: Witter et al., 2017). Second, although activity of a single voxel,
comprised of thousands of neurons, may be considered to be a coarser unit of
analysis than recordings from single units, it may be the case that it is the
operation of a population of these neurons that is most closely linked to
organizational temporal dynamics. It is the gradients revealed by autocorrelation
at the single voxel level that enabled us to link hippocampal dynamics to
behavior. In addition, we were able to segment the populations into clusters,
suggesting subdivisions that would not be evident at the single-unit level. It would
be worthwhile to determine whether similar clusters are found in rodents and
examine their functional significance. Similar analyses at the population-level in
rodents may yield information about the relation of neural dynamics to higher-
level memory representations and goals, an enterprise that is just beginning
(Jacob & Josselyn, 2020; Morrissey et al., 2017).
767
Our results provide compelling evidence for a gradation of single voxel
autocorrelation in the hippocampus and ERC. As predicted, our single voxel
method proved to be a fine-grained measure that revealed subtleties in the
spatial organization of autocorrelation, going beyond prior methods, and allowed
us to observe graded signals along anterior-posterior and medial-lateral axes in
both regions. Further, we show for the first time that differences in single voxel
autocorrelation gradients in the hippocampus can be directly related to
differences in difficulty during a virtual navigation task, thus opening the door for
future research to ask new questions of the autocorrelation signal and uncover
how it is related to behavior.
778
779   **Materials and Methods**
780
Dataset 1: Resting state fMRI
Participants
We analyzed resting state fMRI data from 44 participants (14 male) from the
Human Connectome Project (HCP) Retest dataset. This dataset consists of data
from 44 participants who were scanned twice using the full HCP imaging
protocol. All subject recruitment procedures and informed consent forms,
including consent to share de-identified data, were approved by the Washington
University Institutional Review Board (IRB) (Glasser et al. 2016). The present
analysis of this dataset was approved by the University of Toronto research

ethics board.

Scanning parameters and preprocessing

Resting state data were collected using a multiband EPI pulse sequence (TR =

720 ms, TE = 33.1 ms, 72 slices with 2 mm thickness, FOV = 208 x 180 mm,

voxel size = 2x2 mm, Flip angle = 52, Multiband factor = 8, Scan time = 14

minutes and 33 seconds). Each run was repeated twice, with a left-to-right and a

right-to-left phase encoding direction. The presented results are generated from

data with the left-to-right phase encoding direction.

Initial fMRI preprocessing steps already applied to the downloaded data included

fieldmap correction, motion correction, brain extraction, registration to standard

space, and intensity normalization (Glasser et al., 2013; Smith et al., 2013; Van

Essen et al., 2013). The data were further preprocessed using the FIX tool in

FSL (Griffanti et al., 2014; Salimi-Khorshidi et al., 2014), and noise components

related to head motion and other artifacts were removed. To eliminate high

frequency noise and artifacts, fMRI signals are low-pass filtered using MATLAB

IIR Butterworth filter (designfilt function in Signal Processing Toolbox) with cutoff

frequency of 0.1 Hz.

Single voxel autocorrelation method

Computing single voxel autocorrelation

Bilateral hippocampal and entorhinal masks were generated using the Harvard-

Oxford Atlas in FSL. For each voxel inside each of the regions of interest (ROIs),

unbiased autocorrelation (as implemented in MATLAB xcorr function) was

calculated. Specifically, the timecourse of a single voxel's activity was correlated

with itself shifted by a temporal lag, the length of 1 TR (Dataset 1 TR = 720 ms).

We repeated this process, shifting the timecourse forward by 1 lag (720 ms) and

correlating it with the original, non-shifted timecourse until a maximum temporal

shift of 4 seconds was reached. We chose 4 seconds because it has been shown

that the autocorrelation of the fMRI signal in the gray matter drops off after 4

seconds (i.e., it is not distinguishable from the autocorrelation of other noise)

(Bollmann et al., 2018). For example, the non-shifted timecourse was correlated

with lag 1 (length of 1 TR), lag2 (length of 2 TRs), etc. (Figure 1). The

autocorrelation (AC) computed for each lag was stored in a vector. The

autocorrelation vector (single voxel autocorrelation vector) contained 5 values

(one single voxel autocorrelation for each lag). This approach resulted in a single

voxel autocorrelation vector for each voxel (Figure 1A). All single voxel

autocorrelation values were normalized by subtracting the mean and dividing by

the standard deviation within each mask so that meaningful comparisons could

be made between the two fMRI datasets (resting state and task). Single voxel
autocorrelation maps were then averaged across the first and second runs from
the 44 participants to generate an average overall map (e.g., Figure 1B).
833
Single voxel autocorrelation – Reliability Analysis
To verify that the observed single voxel autocorrelation pattern was not a
measurement artifact (e.g., head motion, magnetic field inhomogeneity,
physiological artifacts, etc.), we tested the reliability of the single voxel
autocorrelation pattern within an individual. In our case, the single voxel
autocorrelation pattern was deemed reliable if there was a high degree of
agreement between the single voxel autocorrelation values generated from
different runs from the same participant compared to runs from different
participants. Reliability of the single voxel autocorrelation values was measured
by calculating the Euclidean distance (ED) between the single voxel
autocorrelation vectors for all pairs of run-wise datasets. 44 participants with 2
repeated sessions produced 44 intra-subject and 3784 inter-subject ED values.
The lower the ED between two single voxel autocorrelation vectors, the higher
the similarity between them. We expected to see more similar single voxel
autocorrelation patterns between single voxel autocorrelation vectors generated
from two runs of the same participant compared to two runs from different
participants (lower intra-subject ED compared to inter-subject ED). The inter-
subject and intra-subject ED are not completely independent from one another,
therefore we used nonparametric permutation to test for significance. We
randomly shuffled the intra-and inter-subject labels and pulled two samples of
size 44 (intra-subject) and 3784 (inter-subject). We calculated the mean
difference between the two samples and repeated this process 10,000 times,
resulting in a histogram of mean differences under the null hypothesis (i.e., the
difference between intra- and -inter-subject ED equal to zero). We compared the
observed difference between intra- and inter-subject EDs with the null distribution
and calculated nonparametric p-values. Permutation tests were conducted using
a permutation testing package in Matlab (Laurens, 2021).
861
Computing single voxel autocorrelation clusters (Autocorrelation Clustering)
The Euclidean distance between the single voxel autocorrelation vectors of each
voxel pair in each mask was calculated to create a distance matrix. The distance
matrix was first normalized (i.e., divided by the maximum value) and then
subtracted from 1 to generate a similarity matrix ranging from 0 to 1. This
similarity matrix was used to generate hippocampal clusters using the modularity
optimization algorithm proposed by (Blondel et al., 2008; Wickramaarachchi et
al., 2014). Unlike the majority of the clustering methods, modularity optimization

does not require to assign the number of clusters and estimates the optimum

number of clusters from data. In addition to clustering at the level of each

individual, group-level clustering was performed by averaging the similarity

matrices of all participants (e.g., Figure 1C).

Autocorrelation Clustering – Reliability Analysis

Reliability of the clustering was measured by calculating the overlap between the

generated clusters using the Jaccard coefficient. The Jaccard coefficient of

regions A and B is defined as:

880
$$J(A, B) = \frac{|A \cap B|}{|A \cup B|}$$

Where $|A \cap B|$ is the number of common voxels in both A and B (intersection)

and $|A \cup B|$ is the number of voxels in A and B combined (union). Individual

parcellations were then compared to the group-level parcellation to examine the

consistency of parcellation. The Jaccard coefficient was calculated both intra-

subject (overlap between clusters extracted from two runs from the *n*th subject)

and inter-subject (overlap between the cluster from the *n*th subject and the same

cluster estimated in all other subjects).

Assuming that the single voxel autocorrelation pattern is consistent across the

two runs of the same participant, we expected there to be greater spatial overlap

(higher Jaccard coefficient) among clusters within an individual compared to

between different individuals. The Jaccard coefficients for clusters within

participants are not completely independent from the Jaccard coefficients for

clusters between participants, therefore we used nonparametric permutation to

test for significance. For each cluster, we randomly shuffled the intra-and inter-

subject labels and pulled two samples of size 44 (intra-subject) and 3784 (inter-

subject). We calculated the mean difference between the two samples and

repeated this process 10,000 times, resulting in a histogram of the mean

differences under the null hypothesis (i.e., the difference between intra- and -

inter-subject Jaccard coefficient equal to zero). We compared the observed

difference between intra- and inter-subject Jaccard coefficients with the null

distribution and calculated nonparametric P values.

Dataset 2: Navigation *fMRI*

Participants

Task fMRI data is from Brunec, Bellana, et al. (2018), where 19 participants (9

males; mean age 22.58 years, range 19-30 years) were scanned while

navigating Google Street View routes around the city of Toronto. All subject

recruitment procedures and informed consent was approved by the University of
Toronto research ethics board.
912
Paradigm
Participants met with the experimenter ahead of time and built routes that were
either highly familiar or less familiar to them (e.g., frequently travelled or not).
Participants then returned to the lab for their second session and were scanned
while they navigated four different types of routes. 1) Familiar: participants
started at a familiar landmark and navigated to a familiar goal destination via a
familiar route, 2) Mirrored: participants started at a familiar landmark and
travelled to a familiar destination via a familiar route, but the images of the route
were mirrored (left-right reversed), 3) Unfamiliar: participants started at a familiar
location, navigated to a familiar destination, but they were instructed to take an
unfamiliar route between the two, and 4) GPS: participants started at an
unfamiliar location in an unfamiliar part of town and pressed arrow keys following
the directions displayed by an arrow on the screen to the goal destination.
Participants completed four unique routes in each condition, sixteen routes in
total (1 route = 1 scanned run). At the end of each route, participants rated the
difficulty of the route on a scale from 1 (difficult) to 9 (easy).
929
Scanning parameters and preprocessing
Participants were scanned with a 3T Siemens MRI scanner at Baycrest's Rotman
Research Institute. A high-resolution 3D MPRAGE T1-weighted pulse sequence
image (160 axial slices, 1 mm thick, FOV = 256 mm) was first obtained to register
functional maps against brain anatomy. Functional imaging was performed to
measure brain activation by means of the blood oxygenation level dependent
(BOLD) effect. Functional T2*-weighted images were acquired using echo-planar
imaging (30 axial slices, 5 mm thick, TR = 2000 ms, TE = 30 ms, flip angle = 70
degrees, FOV = 200 mm). The native EPI resolution was 64 x 64 with a voxel
size of 3.5mm x 3.5mm x 5.0mm. Images were first corrected for head motion
using the Analysis of Functional NeuroImages (AFNI; Cox, 1996). All subsequent
analysis steps were conducted using the statistical parametric mapping software
SPM12.
943
Preprocessing involved slice timing correction, spatial realignment and co-
registration, with a resampled voxel size of 3mm isotropic, with no spatial
smoothing. As all of our analyses rely on covariance, we additionally regressed
out the mean time-courses from participant-specific white matter, and
cerebrospinal fluid masks, alongside estimates of the 6 rigid body motion
parameters from each EPI run. To further correct for the effects of motion which

may persist despite standard processing (Power et al., 2012), an additional
motion scrubbing procedure was added to the end of our preprocessing pipeline.
Using a conservative multivariate technique, time points that were outliers in both
the six rigid-body motion parameter estimates and BOLD signal were removed,
and outlying BOLD signal was replaced by interpolating across neighboring data
points. Motion scrubbing further minimizes any effects of motion-induced spikes
on the BOLD signal, over and beyond standard motion regression, without
leaving sharp discontinuities due to the removal of outlier volumes (for details,
see Campbell et al., 2013). To enable comparisons at the group-level, the final
step of the preprocessing involved warping participants' functional data to the
MNI-space template.
961
Single voxel autocorrelation method
Computing single voxel autocorrelation
To compute the single voxel autocorrelation, we completed the same procedure
outlined in Dataset 1. We used the same bilateral hippocampal masks to extract
the HPC voxels in Dataset 2. For each voxel, the single voxel autocorrelation
was calculated by repeatedly shifting temporal lags (length of 1 TR) until a
maximum lag of 4 seconds was reached. In Dataset 2 the TR was 2000 ms;
therefore, single voxel autocorrelation for 2 lags (or 2 TRs) was calculated,
resulting in a maximum lag of 4 seconds. As outlined in the procedure above,
single voxel autocorrelation values were normalized by subtracting the mean and
dividing by the standard deviation. Single voxel autocorrelation was calculated for
all four runs of each navigational condition (Familiar, Unfamiliar, Mirrored, GPS).
The single voxel autocorrelation was averaged across the four scanned runs
(unique routes), resulting in four different maps (one for each navigational
condition). Single voxel autocorrelation maps were then averaged across the 19
participants to generate an average group map for each navigation condition.
978
Participants completed 16 navigation runs (four in each condition) at their own
pace. Because the conditions varied in difficulty, the average number of TRs
differed across conditions and participants. Every route was 2-10 km long and
the average run (route) length was 137.6 TRs (2 s TRs). The average number of
TRs was lowest in the GPS condition (M = 92.13, SD = 17.44), followed by the
Familiar condition (M = 136.45, SD = 39.18), the Mirrored condition (M = 155.73,
SD = 36.84), and the Unfamiliar condition (M = 158.78, SD = 32.13). In order to
compare single voxel autocorrelation across scanned runs with a similar number
of TRs/lengths, we chose to filter out any runs that were unusually short (that the
participant either didn't complete or completed very quickly). We excluded runs
that were less than 88 TRs long. This resulted in an average of 13.36 runs (SD =

1.21) per participant. The GPS runs were disproportionately shorter than the
other conditions, resulting in more GPS runs excluded than other conditions. The
average number of routes included in the following analyses per participant are
as follows: Mirrored (M=3.89, SD=0.31), Unfamiliar (M=3.84, SD=0.50), Familiar
(M=3.68, SD=0.47), GPS (M=1.95, SD=1.22).
995
996   *Computing autocorrelation clusters (Autocorrelation Clustering)*
997   We repeated the single voxel autocorrelation clustering procedure described
998   above in Dataset 1 to determine clusters of single voxel autocorrelation within
999   each navigational condition.
1000
Relating single voxel autocorrelation to navigation condition
Calculating single voxel autocorrelation slopes
To investigate how the spatial distribution of single voxel autocorrelation is
related to navigation difficulty, we compared the single voxel autocorrelation (lag
1) slopes across the four different conditions: GPS, Familiar, Unfamiliar, and
Mirrored. First, for each participant, we extracted the single voxel autocorrelation
(lag 1) from every voxel. We averaged the single voxel autocorrelation across all
voxels on each slice of the hippocampus. We used 3 mm slices in the anterior-
posterior direction (Y-direction), resulting in thirteen slices. Using a linear
regression, we calculated the slope coefficient for the single voxel autocorrelation
across slices for each navigation run. We then repeated the same procedure,
using 3 mm slices in the medial-lateral direction (X-direction), resulting in 9
slices. We computed the slopes and compared them across navigation
conditions and hemispheres.
1015
To test whether there was a significant difference between single voxel
autocorrelation during different navigation conditions, we ran a mixed effects
model on the single voxel autocorrelation slopes along the anterior-posterior and
medial-lateral axes. This analysis was conducted in R (R Core Team, 2019)
using the afex (Singmann et al., 2020) and the tidyverse packages (Wickham,
2017).

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