

Title: Single voxel autocorrelation uncovers gradients of temporal dynamics in the hippocampus and entorhinal cortex during rest and navigation

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Abstract

During navigation, information at multiple scales needs to be integrated. Single-unit recordings in rodents suggest that gradients of temporal dynamics in the hippocampus and entorhinal cortex support this integration. In humans, gradients of representation are observed, such that granularity of information represented increases along the long axis of the hippocampus. The neural underpinnings of this gradient in humans, however, are still unknown. Current research is limited by coarse fMRI analysis techniques that obscure the activity of individual voxels, preventing investigation of how moment-to-moment changes in brain signal are organized and how they are related to behavior. Here, we measured the signal stability of single voxels over time to uncover previously unappreciated gradients of temporal dynamics in the hippocampus and entorhinal cortex. Using our novel, single voxel autocorrelation technique, we show for the first time a medial-lateral hippocampal gradient, as well as a continuous autocorrelation gradient along the anterolateral-posteromedial entorhinal extent. Importantly, we show that anterior-posterior and medial-lateral hippocampal autocorrelation gradients were modulated by navigational difficulty, indicating that changes in signal stability are relevant for behavior. Our method and findings open the door for future research on how temporal gradients within these structures support the integration of information for goal-directed behavior.

Acknowledgments

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Conflict of interest statement

The authors declare no competing financial interests.

1 **Introduction**

2

3 To enable efficient goal-directed behaviour, information must be represented and
4 integrated across multiple temporal and spatial scales. It has been proposed that
5 neural signal gradients in the hippocampus and entorhinal cortex support such
6 multi-scale representations in rodents, but evidence in humans is sparse and has
7 methodological limitations. Previously, fMRI analysis techniques have uncovered
8 local signal gradients in the human hippocampus (Brunec, Bellana, et al., 2018).
9 These investigations, however, have been limited by analyzing patterns of
10 activity across relatively coarse regions of interest, making it unclear how
11 sustained versus rapidly changing signals are distributed throughout the
12 hippocampus. Many of these analyses use predetermined anterior and posterior
13 anatomical masks, which limit our ability to detect neural signal gradients in an
14 unsupervised way, therefore preventing us from investigating gradients that exist
15 along both anterior-posterior and medial-lateral axes of the hippocampus.
16 Moreover, there have been no prior investigations of autocorrelation gradients in
17 the entorhinal cortex, despite evidence of its role in spatial and temporal
18 representations during navigation. To address these limitations, we have
19 developed a novel, data-driven analysis based on autocorrelation of single voxels
20 in fMRI during rest and navigation. This technique allows us, for the first time, to
21 track the signal stability of individual voxels and their spatial distribution in an
22 unconstrained way along both the anterior-posterior and medial-lateral axes of
23 the hippocampus and entorhinal cortex. Based on this single voxel analysis we
24 uncover gradients of neural signal dynamics along these axes in both structures
25 and relate them to behavior.

26

27 In rodents, place fields in the ventral hippocampus (homologous to the anterior
28 hippocampus in humans) span larger areas, show a higher degree of overlap,
29 and higher correlation in their firing across time, compared to the dorsal
30 hippocampus (homologous to the posterior hippocampus in humans) (Hasselmo,
31 2008; Jung et al., 1994; Kjelstrup et al., 2008; Komorowski et al., 2013). A similar
32 gradient of hippocampal organization is also observed in the human
33 hippocampus. Tracking moment-to-moment similarity across patterns of voxels
34 during virtual navigation, Brunec, Bellana, et al. (2018) found that signal similarity
35 was significantly greater within the anterior hippocampus relative to the posterior
36 hippocampus, indicating that, as in the rodent ventral hippocampus, the human
37 anterior hippocampus demonstrates slower changing signals that are sustained
38 across time and space. These results suggest that a relatively stable pattern of
39 activity in the rodent and human hippocampus follows a scaled gradient, from
40 faster changing signal in the posterior (dorsal) hippocampus to slower changing

41 signal in the anterior (ventral) hippocampus. This gradient organization might
42 underlie fine-to-coarse mnemonic representation, particularly when a different
43 granularity of information needs to be maintained across time (Brunec &
44 Momennejad, 2019; Robin & Moscovitch, 2017). In addition to the dorsal-ventral
45 gradient of spatial representation observed in rodents, research suggests a
46 difference in spatial selectivity along the proximodistal axis (homologous to
47 medial-lateral in humans), specifically in CA1 (Igarashi et al., 2014), yet whether
48 a similar medial-lateral distinction exists in the human hippocampus is still
49 unclear (Hrybouski et al., 2019).

50

51 A key input structure to the hippocampus that has been implicated in integrating
52 information over time during navigation is the entorhinal cortex. Prior research
53 has found distinct functional differentiation between the anterolateral and
54 posterior-medial aspects of the entorhinal cortex (ERC), but there have been no
55 prior investigations of neural signal gradients in the ERC. The lateral ERC in
56 rodents, and the homologous anterolateral ERC in humans, supports within-
57 object and object-location coding, as well as temporal information processing
58 (Bellmund et al., 2019; Montchal et al., 2019; Olsen et al., 2017; Tsao et al.,
59 2018; Yeung et al., 2017; 2019). In contrast, the posteromedial ERC in humans,
60 has been primarily linked to scene processing (Berron et al., 2018; Maass et al.,
61 2015; Navarro Schröder et al., 2015) and related to grid cell organization
62 (Bellmund et al., 2016), consistent with evidence of grid cells in the medial ERC
63 in rodents (Hafting et al., 2005). Given prior evidence of functional distinctions of
64 the ERC into anterolateral and posteromedial regions, we developed a data-
65 driven method to investigate directly, a continuous neural signal gradient in both
66 the anterior-posterior and medial-lateral axes of this structure.

67

68 To understand how a graded organization of signal dynamics in the hippocampus
69 and ERC supports goal-directed behavior, we developed an analytic approach of
70 temporal autocorrelation at the single voxel level, which we implemented during
71 both rest and navigation. Temporal autocorrelation represents the degree of
72 similarity between a signal and the temporally shifted, or lagged, version of the
73 signal over successive time intervals (Figure 1A). Conventionally, it is assumed
74 that this autocorrelation in fMRI data originates from physical and physiological
75 noise (Arbabshirani et al., 2014; Bollmann et al., 2018; Bullmore et al., 2001;
76 James et al., 2019; Lenoski et al., 2008; Lund et al., 2006; Purdon & Weisskoff,
77 1998) or the hemodynamic response function (Arbabshirani et al., 2014; James
78 et al., 2019; Rajapakse et al., 1998) and, therefore, has been considered
79 irrelevant to brain function. Recently, however, Arbabshirani et al. (2019) found
80 that autocorrelation reflects changes in cognitive state (task vs. rest) as well as

81 changes in mental state (healthy control vs. schizophrenia), suggesting that the
82 observed changes in the autocorrelation are also modulated by cognitive
83 processes. Prior studies, however, have been limited and are unable to answer
84 the question of how temporal autocorrelation is directly related to behavior.
85 Examining the temporal autocorrelation of single voxels during an active
86 navigation task, therefore, is important for understanding how a stable, highly
87 correlated signal is relevant for behavior.

88

89 Investigating the fMRI signal at the single voxel level allows us to measure neural
90 gradients with more precision than previous methods. While studies with fMRI in
91 humans suggest that functional heterogeneity exists along the long axis of the
92 hippocampus (Nadel et al., 2013; Poppenk et al., 2013; see Grady, 2020 for a
93 review) and medial-lateral extent of the ERC (e.g., Hafting et al., 2005; Maass et
94 al., 2015; Navarro Schröder et al., 2015), previous analysis techniques have
95 been limited to investigations using predetermined anatomical masks, which
96 obscures the contribution of individual voxels, making it unclear whether graded
97 signals extend along multiple axes in these regions. Furthermore, examining the
98 autocorrelation at the single voxel level allows for a finer-grained analysis that
99 may be more sensitive to differences in navigational performance and can help
100 us to determine how a scaled gradient of signal similarity might be employed to
101 integrate representations across spatial scales during navigation. We, therefore,
102 combine our single voxel autocorrelation approach with an unconstrained
103 clustering method to determine how temporal autocorrelation is distributed in
104 multiple dimensions throughout the hippocampus and ERC.

105

106 Here we present the first evidence of a medial-lateral neural signal gradient in the
107 hippocampus as well as a novel continuous gradient in the ERC. Using resting
108 state fMRI data with high spatial and temporal resolution from the Human
109 Connectome Project (HCP), we measured single voxel autocorrelation in the
110 hippocampus and ERC. Specifically, we measured the similarity of single voxels
111 over time by correlating the timecourse of each voxel with temporally shifted
112 versions of itself (Figure 1A). We applied data-driven clustering to determine how
113 temporal autocorrelation was spatially distributed throughout the hippocampus
114 and ERC. We found high autocorrelation in the anterior-medial hippocampus and
115 posteromedial ERC and low autocorrelation in the posterior-lateral hippocampus
116 and anterolateral ERC. Using task-based fMRI, we replicated these results and
117 also demonstrated that increases in navigation difficulty were associated with
118 increases in autocorrelation in the anterior-medial hippocampus. Our single voxel
119 autocorrelation approach yields consistent and precise gradients of single voxel
120 autocorrelation in the hippocampus and ERC, providing a powerful new

121 continuous and data-driven method that can illuminate how temporal dynamics in
122 brain signals relate to complex cognition.

123

124 **Results**

125

126 **Dataset 1: Resting state fMRI**

127 **Hippocampus**

128 ***Spatial distribution of single voxel autocorrelation***

129 To examine hippocampal dynamics at the single voxel level when no cognitive
130 demands were placed on participants, we first analyzed resting-state fMRI data
131 from 44 participants from the Human Connectome Project (HCP) Retest dataset
132 (2 runs per participant). Here, we correlated the timecourse of activity of each
133 voxel in the hippocampus with activity in that same voxel shifted by a temporal
134 lag of 1 TR (Dataset 1 TR = 720 ms). We repeated this process until a maximum
135 temporal shift of 4 seconds was reached, or 5 lags (Figure 1A). A map of single
136 voxel autocorrelation values throughout the hippocampus was generated for
137 each lag separately (for a theoretical schematic, see Figure 1B).

138

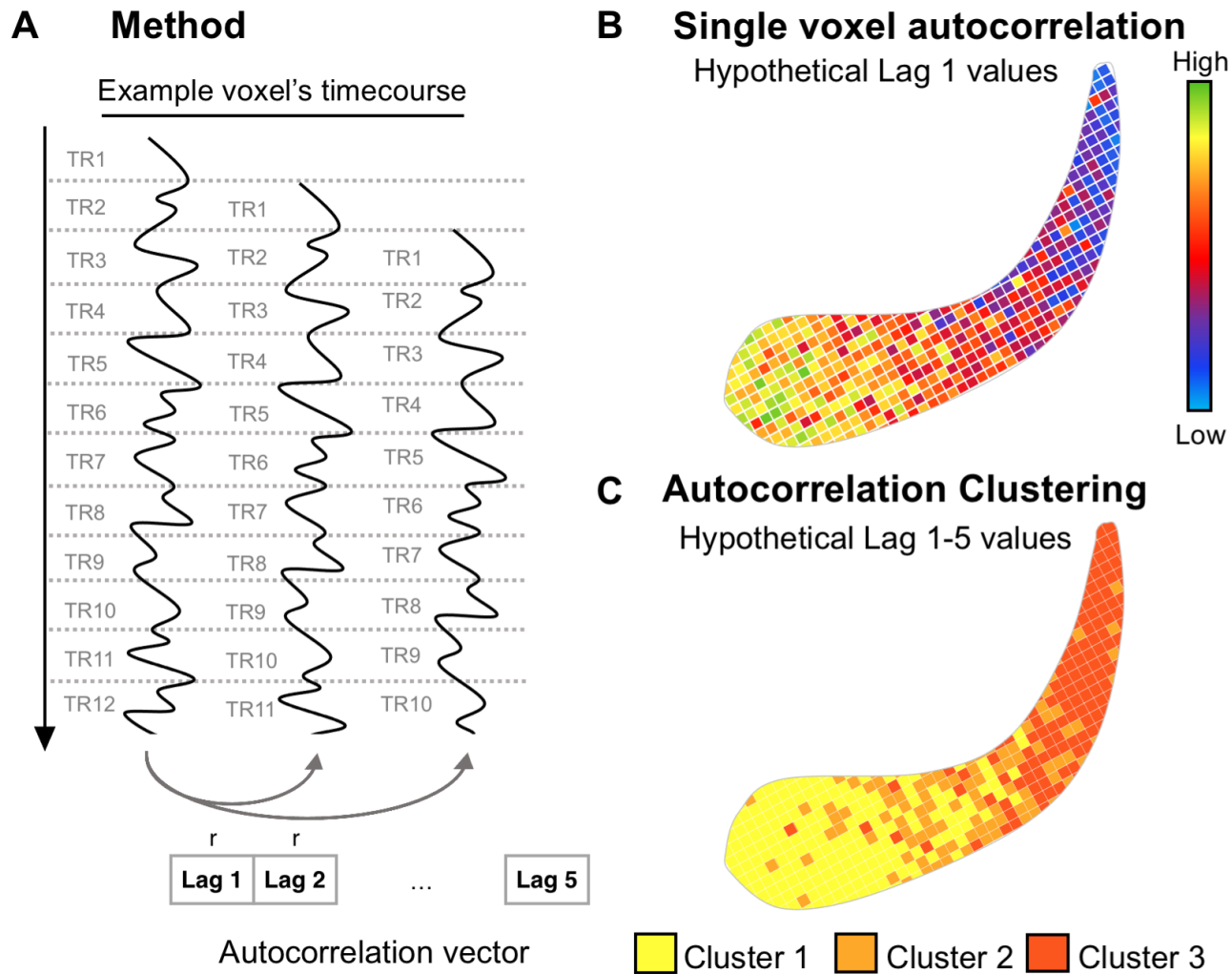
139 We found that single voxel autocorrelation maps at the group level (lags 1-5)
140 showed a notable difference in the distribution of single voxel autocorrelation
141 values along the hippocampal axis (Figure 2A). More specifically, voxels with
142 higher single voxel autocorrelation were mainly in the anterior-medial region
143 whereas voxels with lower single voxel autocorrelation were mainly in the
144 posterior-lateral region (in both left and right hippocampus). As shown in Figure
145 2A, although the overall autocorrelation decreased as the lag increased, the
146 overall pattern of autocorrelation gradients was similar for lags 1-5.

147

148 ***Single voxel autocorrelation – Reliability results***

149 We next tested the reliability of these results. Here we defined a reliable result as
150 one in which single voxel autocorrelation vectors generated from two runs of the
151 *same* participant were more similar than two runs from *different* participants
152 (lower intra-subject Euclidean distances compared to inter-subject Euclidean
153 distances). Nonparametric permutation tests comparing intra-subject and inter-
154 subject Euclidean distance revealed reliable results in both the left (intra-subject:
155 7.43 ± 2.07 , inter-subject: 9.38 ± 2.22 , $P < 0.0001$) and right hippocampus (intra-
156 subject: 7.22 ± 1.98 , inter-subject: 9.02 ± 2.02 , $P < 0.0001$) (Figure 3A). These
157 high intra-subject similarity values suggest that the single voxel autocorrelation
158 pattern is an intrinsic feature of the brain, likely originating from neuronal
159 sources, rather than noise or imaging artifacts.

160



162

163 **Figure 1. A) Method.** For each voxel, the timecourse of activity was successively
 164 temporally shifted by 1 TR and correlated with itself. This was repeated for a total shift of
 165 4 seconds (i.e., 5 lags for resting state data (Dataset 1) and 2 lags for navigation data
 166 (Dataset 2)). This resulted in a vector of single voxel autocorrelation values, with each
 167 value corresponding to a different lagged correlation. **B) Single voxel autocorrelation**
 168 **(hypothetical values).** The procedure was repeated for all voxels in an ROI. To
 169 examine the spatial distribution of the single voxel autocorrelation, we plot the group-
 170 level single voxel autocorrelation maps for each lag, averaged across runs and
 171 participants. **C) Autocorrelation clustering (hypothetical values).** The autocorrelation
 172 values for each lag were stored in a vector (single voxel autocorrelation vector). The
 173 voxels in the ROI were clustered based on the similarity (Euclidean distance) of single
 174 voxel autocorrelation vectors. Single voxel autocorrelation vectors were clustered
 175 according to their Euclidean distance (Blondel et al., 2008). Clustering was performed at
 176 the individual-level and at the group-level.

177

178 **Autocorrelation Clustering**

179 We applied a Louvain clustering method using modularity maximization without
180 predefining the number of clusters (Blondel et al., 2008) to the group-level single
181 voxel autocorrelation vectors (for a theoretical schematic, see Figure 1C). This
182 data-driven clustering approach revealed three distinct clusters in both the left
183 and right hippocampus (Figure 2B); notably, past work that segmented the
184 hippocampus into two ROIs (anterior and posterior) a priori would not have been
185 able to detect the presence of this third cluster. Consistently across all 5 lags we
186 found that Cluster 1 had the highest single voxel autocorrelation values and was
187 located in the anterior-medial hippocampus (Figure 2D). Cluster 3 had the lowest
188 single voxel autocorrelation values and was located in the posterior-lateral part of
189 the hippocampus. Cluster 2 had intermediate single voxel autocorrelation values
190 and was located between Clusters 1 and 3. These three clusters were also
191 reliably observed at the individual level (cluster maps from two runs of an
192 example participant are shown in Figure 2B).

193

194 In summary, clustering revealed a high-to-low single voxel autocorrelation
195 gradient along the anterior-posterior axis, consistent with what has been
196 previously found in the literature (Brunec, Bellana, et al., 2018; Raut et al., 2020).
197 In addition, we found differences along the medial-lateral axis, as well as a
198 prominent anterior-medial cluster of high single voxel autocorrelation that could
199 be distinguished from a posterior-lateral cluster of low single voxel
200 autocorrelation. While previous methods using predetermined anterior/posterior
201 ROI masks might have missed this medial-lateral distinction, our data-driven
202 method provides evidence that an autocorrelation gradient exists along multiple
203 spatial dimensions.

204

205 **Autocorrelation Clustering – Reliability results**

206 The reliability of single voxel autocorrelation clustering was evaluated by
207 measuring spatial overlap between clusters, calculated by the Jaccard coefficient
208 (Figure 3B). Here we defined a reliable result as one in which the spatial
209 distribution of autocorrelation clusters was consistent across the two runs of the
210 same participant, indicated by greater overlap (higher Jaccard coefficient) among
211 clusters *within* an individual compared to *between* different individuals. Using
212 nonparametric permutation, we found high reliability for clusters in the bilateral
213 hippocampus, specifically Cluster 1 (Left: $P < 0.001$; Right: $P < 0.001$) and
214 Cluster 3 (Left: $P < 0.001$; Right: $P < 0.001$). These findings of high intra- and
215 inter-subject overlap suggest that Clusters 1 and 3 were highly reliable, within
216 individuals. Cluster 2, however, had significantly lower overlap (Left: $P = 0.06$;
217 Right: $P = 0.007$), suggesting more variability within individuals.

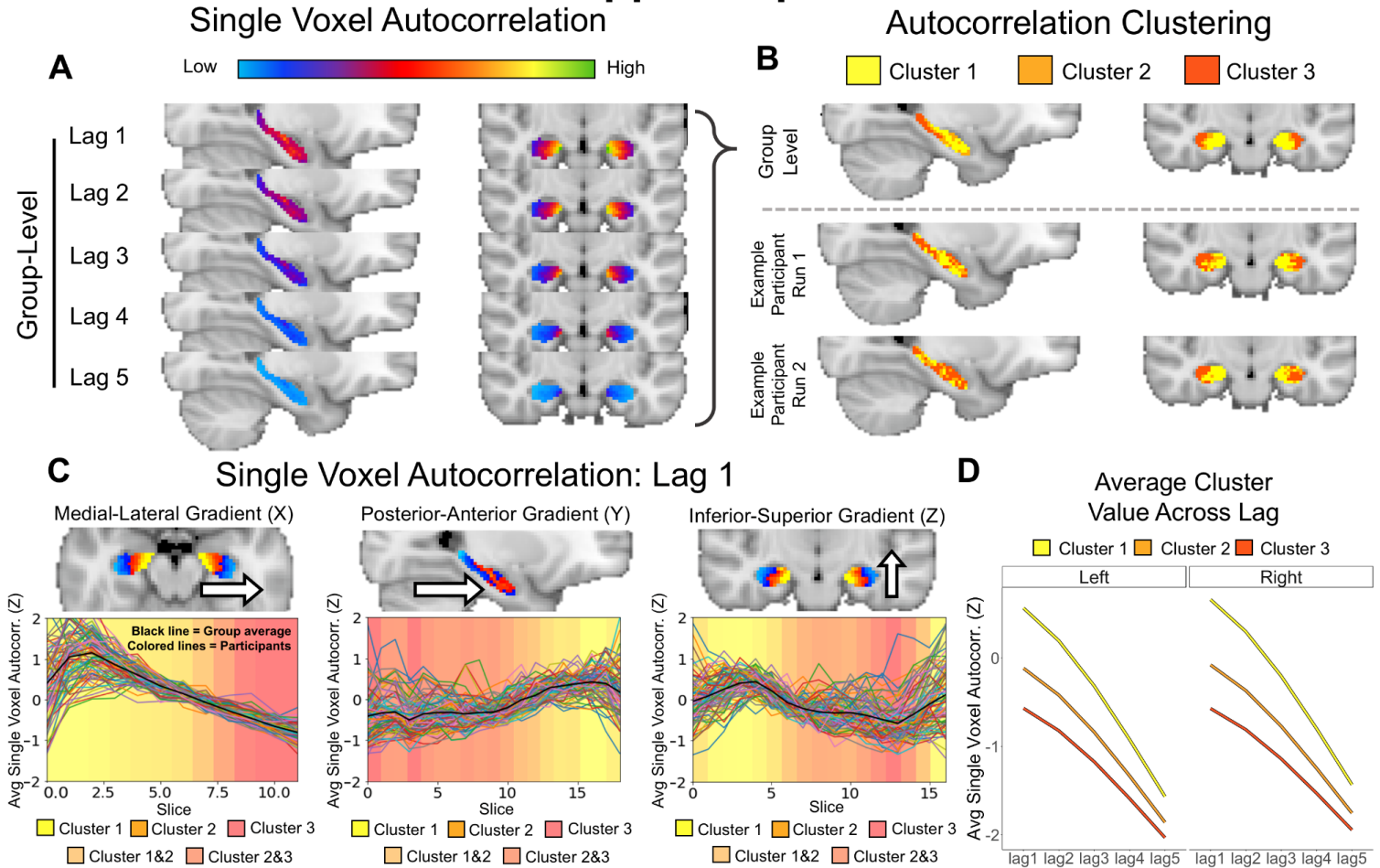
218 ***Gradients of single voxel autocorrelation (lag 1)***

219 The single voxel autocorrelation and autocorrelation clustering results presented
220 above both suggest the presence of an autocorrelation gradient along two main
221 axes: the anterior-posterior axis and the medial-lateral axis. To more precisely
222 examine these individual gradients, we plotted the single voxel autocorrelation
223 across hippocampal slices along the X (medial-lateral), Y (posterior-anterior), and
224 Z (inferior-superior) axes. We observed consistent gradients in every participant.
225 Specifically, single voxel autocorrelation gradually decreased in the medial-to
226 lateral direction and increased in the posterior-to-anterior direction (Figure 2C;
227 we focused on lag 1, but a similar pattern was revealed across all lags, as shown
228 in Figure 2A). A rough gradient of high-to-low autocorrelation was also observed
229 in the inferior-superior axis, which is due to the angle of the hippocampus (i.e.,
230 the anterior hippocampus is located more inferiorly relative to the posterior
231 hippocampus). When we investigated the spatial distribution of the three clusters
232 (projected on the background of the plots in Figure 2C), we observed a gradient
233 of cluster assignment that complemented the single voxel autocorrelation
234 gradients. Specifically, high-to-low single voxel autocorrelation gradients were
235 also associated with a cluster gradient from Cluster 1 to Cluster 3.

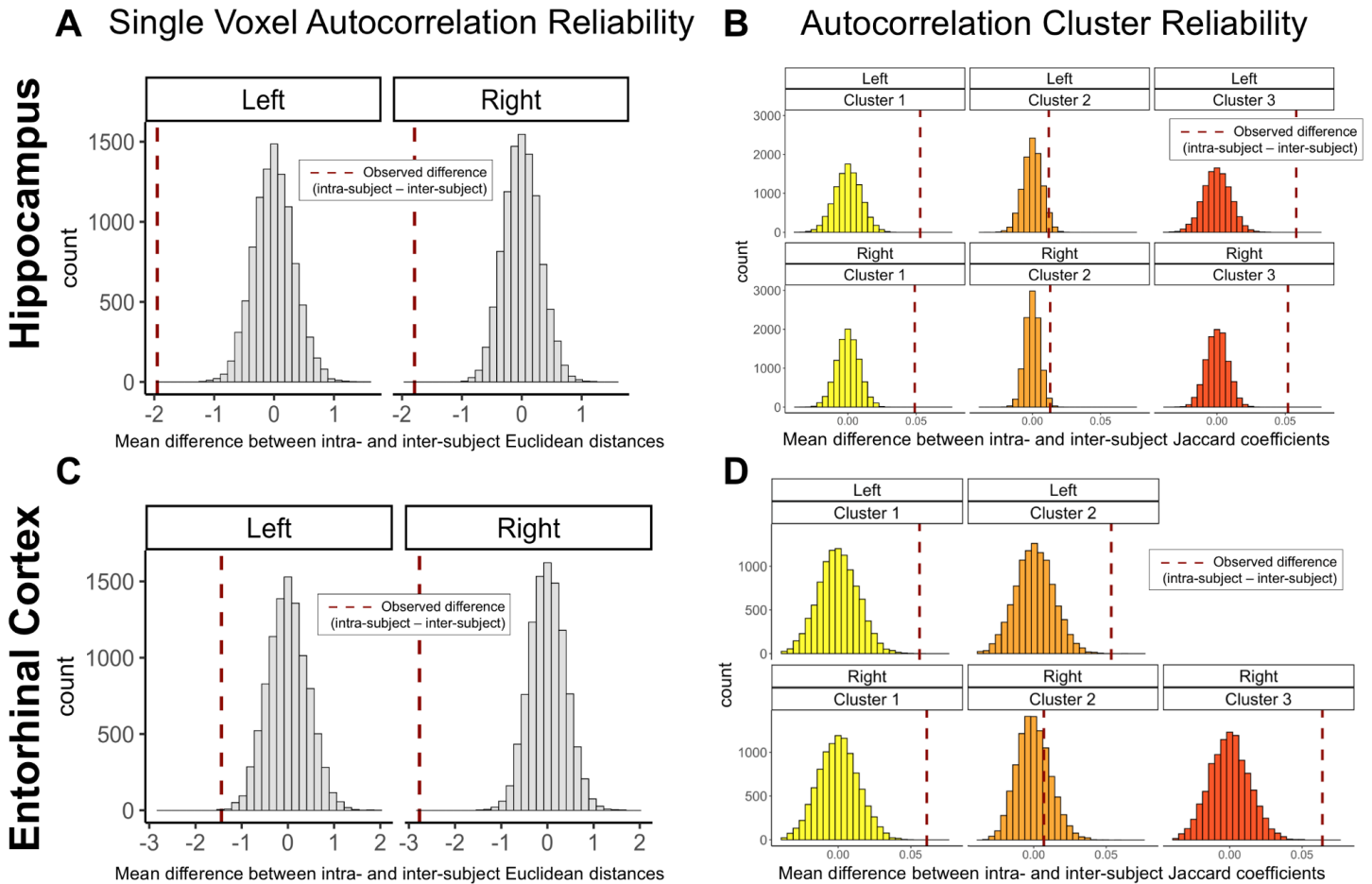
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237

Hippocampus



239 **Figure 2. Hippocampus. Single Voxel Autocorrelation.** **A)** Group-level single voxel
 240 autocorrelation maps averaged across all runs for all participants. **Autocorrelation**
 241 **Clustering.** **B)** Group-level clusters (top) and run-level cluster maps for two runs from an
 242 example participant (bottom). Three distinct clusters were found at both the group and
 243 the individual run-level. Cluster 1 was located in the anterior-medial hippocampus,
 244 Cluster 3 was located in the posterior-lateral hippocampus, and Cluster 2 was located
 245 between Cluster 1 and 3. **C) Single Voxel Autocorrelation: Lag 1.** Single voxel
 246 autocorrelation (lag 1) averaged per slice and projected into three axes (X, Y, and Z) to
 247 visualize changes in medial-lateral, anterior-posterior, and inferior-superior directions
 248 (plots depict left hemisphere; right hemisphere looked similar). The average cluster
 249 assignment of voxels on each slice is presented as the background color to show the
 250 gradation in values along the three axes. **D) Average Cluster Value Across Lag.**
 251 Average group-level single voxel autocorrelation values for each cluster at each lag.
 252 Cluster 1 was associated with the highest single voxel autocorrelation values, Cluster 2
 253 with intermediate values, and Cluster 3 with the lowest. This was consistent across all 5
 254 lags.
 255



257 **Figure 3. Hippocampal and Entorhinal cortex reliability measures. A,C) Single**
 258 **Voxel Autocorrelation Reliability.** Distribution of shuffled and permuted mean
 259 difference of intra- and inter-subject Euclidean distances for the (A) hippocampus and
 260 (C) entorhinal cortex. Dashed lines represent the observed mean difference between
 261 intra- and inter-subject Euclidean distance. Significant negative values indicate that
 262 single voxel autocorrelation values were more similar within an individual than across
 263 individuals. **B, D) Autocorrelation Cluster Reliability.** Distribution of shuffled and
 264 permuted mean difference of intra- and inter-subject Jaccard coefficients for each
 265 cluster. Dashed lines represent the observed difference between intra- and inter-subject
 266 Jaccard coefficients for each cluster. (B) In both hemispheres of the hippocampus,
 267 Clusters 1 and 3 were more reliable within individuals compared to Cluster 2. (D) In the
 268 entorhinal cortex, Cluster 1 and Cluster 2 were reliable within individuals in the left
 269 hemisphere, whereas Cluster 1 and 3 were reliable within individuals in the right
 270 hemisphere.

271
 272
 273
 274
 275

276 **Entorhinal cortex**

277 ***Spatial distribution of single voxel autocorrelation***

278 We repeated the analyses above in the ERC. To illustrate the distribution of
279 autocorrelation values of individual voxels throughout the ERC, we plotted the
280 group-level single voxel autocorrelation maps for lags 1-5 (Figure 4A). The maps
281 illustrate a difference in single voxel autocorrelation throughout the ERC.
282 Specifically, voxels with higher single voxel autocorrelation were mainly in the
283 posterior-medial region whereas voxels with lower single voxel autocorrelation
284 were mainly in the anterior-lateral region (in both left and right ERC).

285

286 ***Single voxel autocorrelation – Reliability results***

287 Nonparametric permutation tests comparing intra-subject and inter-subject
288 Euclidean distance revealed reliable results in both the left (intra-subject: $11.43 \pm$
289 3.64 , inter-subject: 12.87 ± 2.83 , $P < 0.001$ and right ERC (intra-subject: $10.41 \pm$
290 2.63 , inter-subject: 13.19 ± 2.53 , $P < 0.001$; Figure 3C). This analysis
291 demonstrates the reliability of the single voxel autocorrelation and suggests that
292 single voxel autocorrelation patterns between vectors generated from two runs of
293 the *same* participant were more similar than two runs from *different* participants
294 (lower intra-subject Euclidean distances compared to inter-subject Euclidean
295 distances).

296

297 ***Autocorrelation Clustering***

298 The group-level clustering analysis on the voxels within the ERC revealed two
299 distinct clusters in the left hemisphere and three clusters in the right (Figure 4B).
300 For comparison, cluster maps from two runs of an example participant are shown
301 in Figure 4B. Cluster 1 was located in the posteromedial ERC and had the
302 highest single voxel autocorrelation values in both left and right hemispheres.
303 Cluster 2 was observed in the left hemisphere and was located towards the
304 anterior-lateral ERC with low single voxel autocorrelation values. In the right
305 hemisphere it was an intermediate cluster. Cluster 3 was only observed
306 consistently in the right hemisphere and was located in the anterior-lateral ERC
307 with the lowest single voxel autocorrelation values. We computed the group-level
308 single voxel autocorrelation for each cluster and plotted it across all 5 lags
309 (Figure 4D). Across all 5 lags, Cluster 1 consistently had the highest single voxel
310 autocorrelation values, followed by Cluster 2 and Cluster 3.

311

312 ***Autocorrelation Clustering – Reliability results***

313 The reliability measure for ERC clusters was calculated by the Jaccard
314 coefficient (Figure 3D). Nonparametric permutation tests comparing intra-subject
315 and inter-subject cluster overlap revealed reliable results in the left and right

316 hemisphere. In the left hemisphere, the Cluster 1 ($P < 0.001$) and Cluster 2 ($P <$
317 0.001) were reliable. In the right hemisphere, Cluster 1 ($P < 0.001$) and Cluster 3
318 ($P < 0.001$) were reliable. This suggests that these clusters were highly reliable
319 within individuals. In the right hemisphere, Cluster 2 had very small Jaccard
320 values, suggesting less reliability within individuals (Right: $P = 0.53$).

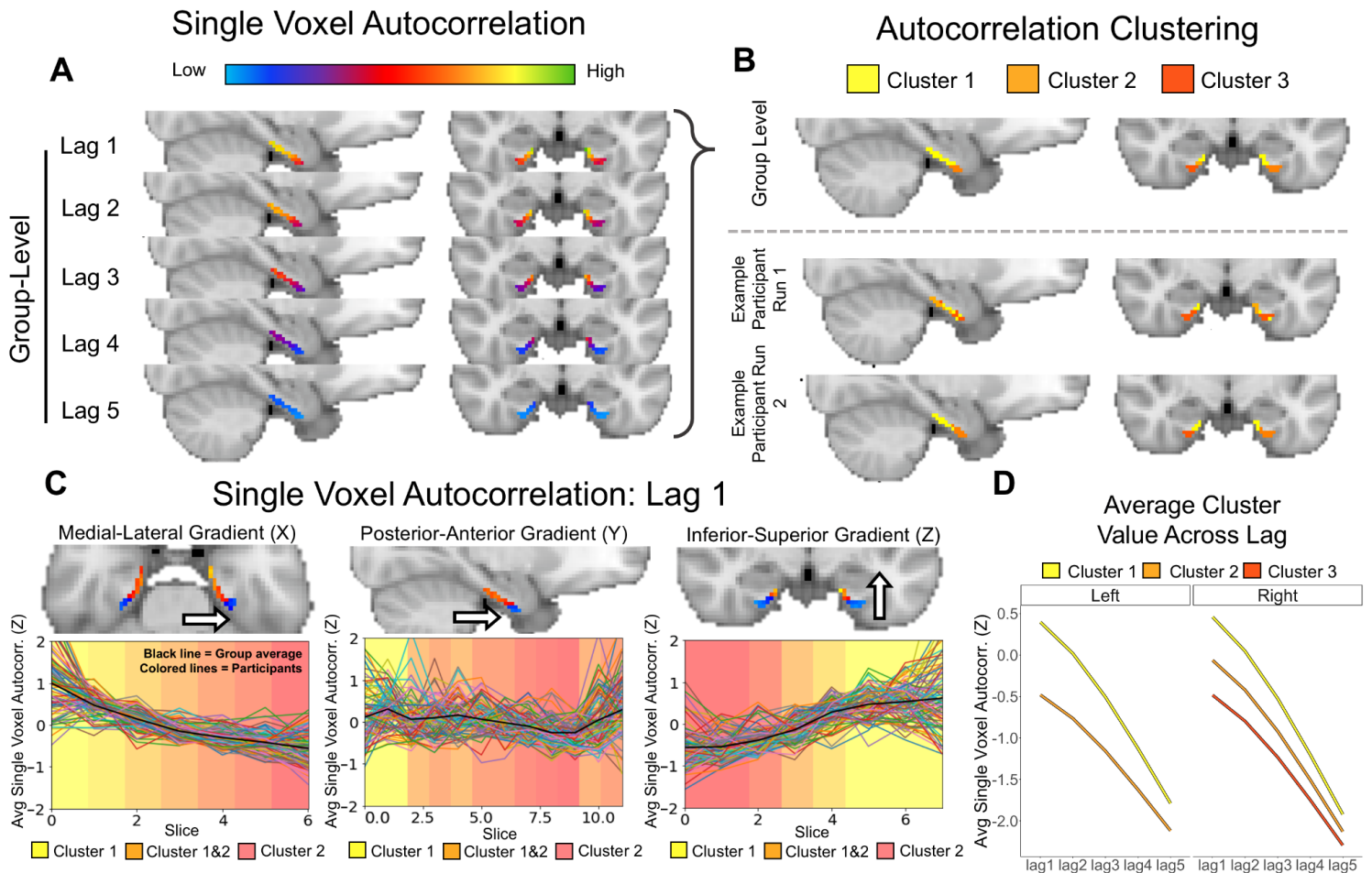
321

322 ***Gradients of single voxel autocorrelation (lag 1)***

323 Single voxel autocorrelation values for lag 1 were projected onto X (medial-
324 lateral), Y (posterior-anterior), and Z (inferior-superior) axes. As shown in Figure
325 4C, in every participant, single voxel autocorrelation values gradually decreased
326 in the medial-to-lateral direction and the posterior-to-anterior direction (Figure
327 4C). We found a gradient of low-to-high autocorrelation along the inferior-
328 superior axis, which is due to the fact that the posterior region of the ERC is more
329 superior than its anterior region. We observed a gradient of cluster assignment
330 that complemented the single voxel autocorrelation gradients, where high-to-low
331 gradients were also associated with a cluster gradient from Cluster1 to Cluster 2.

332

Entorhinal Cortex



334 **Figure 4. Entorhinal cortex. Single Voxel Autocorrelation. A)** Group-level single
 335 voxel autocorrelation maps averaged across all runs for all participants. **Autocorrelation**
 336 **Clustering. B)** Group-level clusters (top) and run-level cluster maps for two runs from an
 337 example participant (bottom). Two distinct clusters were found in the left hemisphere and
 338 three in the right hemisphere. In the left hemisphere, Cluster 1 was located in the
 339 posterior-medial ERC and Cluster 2 was in the anterior-lateral ERC. In the right
 340 hemisphere Cluster 1 was located in the posterior-medial ERC, Cluster 3 was located in
 341 the anterior-lateral ERC, and Cluster 2 was located between Cluster 1 and 3. **C) Single**
 342 **Voxel Autocorrelation: Lag 1.** Single voxel autocorrelation projected below onto three
 343 axes (X, Y, and Z) to visualize changes in medial-lateral, anterior-posterior, and inferior-
 344 superior directions (for the left hemisphere; right hemisphere looked similar). The
 345 average cluster assignment of voxels on each slice is presented as the background color
 346 to show the gradation in values along the three axes (Note the gradation depicts only
 347 Cluster 1 and 2 as there were only two significant clusters found in the left hemisphere).
 348 **D) Average Cluster Value Across Lag.** Average group-level single voxel
 349 autocorrelation values for each cluster at each lag. In the left hemisphere, Cluster 1 was
 350 associated with the highest single voxel autocorrelation values and Cluster 2 with low
 351 autocorrelation values. In the right hemisphere, Cluster 1 was associated with the

352 highest single voxel autocorrelation, Cluster 2 with intermediate values, and Cluster 3
353 with the lowest. This was consistent across all 5 lags.

354

355 **Dataset 2: Navigation fMRI**

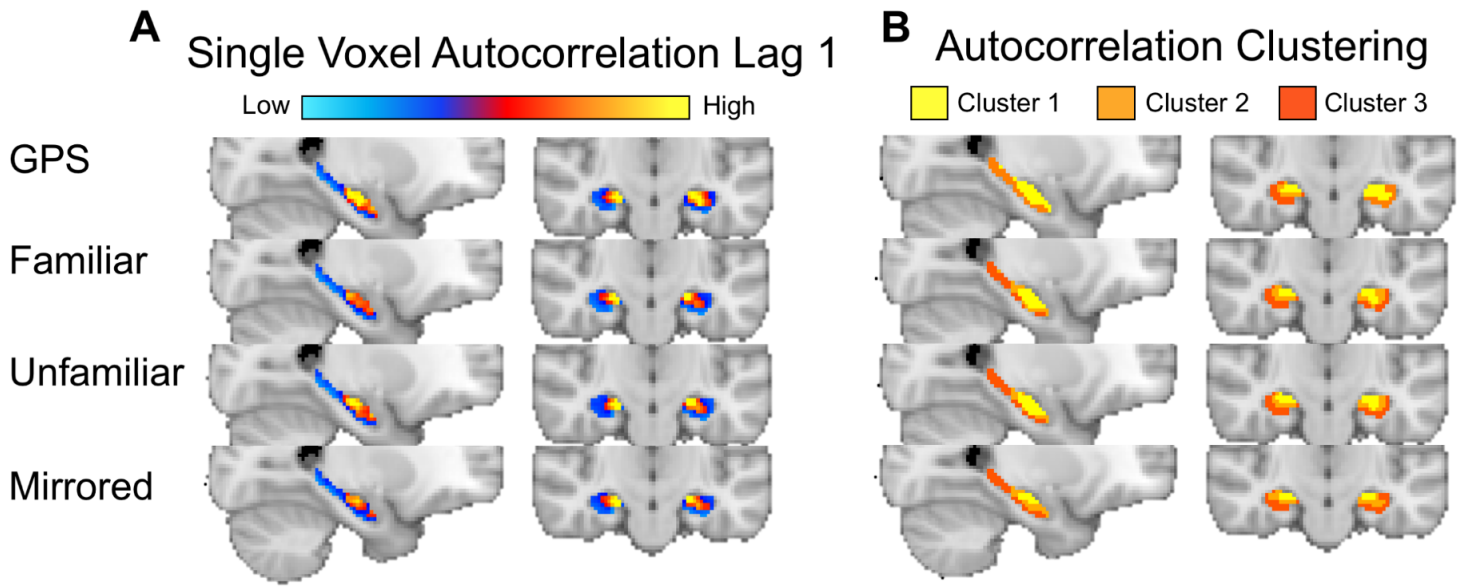
356 We next aimed to replicate the observed effects in task fMRI and relate changes
357 in single voxel autocorrelation to behavior. Specifically, we were interested in
358 how single voxel autocorrelation throughout the hippocampal long axis might be
359 modulated by differences in difficulty during a temporally-extended navigation
360 task. Therefore, we performed our single voxel autocorrelation analyses on a
361 task fMRI dataset acquired while participants navigated in a familiar virtual reality
362 environment (previously described in Brunec, Bellana et al., 2018). Here, 19
363 participants were scanned while navigating Google Street View routes around
364 the city of Toronto. Participants navigated four different types of routes that
365 varied in their navigational difficulty: GPS (unfamiliar routes guided by an arrow),
366 Familiar (highly familiar routes), Unfamiliar (routes that were less familiar), and
367 Mirrored (familiar routes that were left-right reversed). Participants completed
368 four unique routes in each condition, sixteen routes in total (1 route = 1 scanned
369 run). Due to the lower spatial resolution in this dataset we were not able to
370 examine the ERC and, thus, these analyses focused only on the hippocampus.

371

372 **Hippocampus**

373 ***Spatial distribution of single voxel autocorrelation***

374 To compute the single voxel autocorrelation, we completed the same procedure
375 outlined in Dataset 1. In Dataset 2 the TR was 2000 ms; therefore, single voxel
376 autocorrelation for 2 lags (or 2 TRs) was calculated. We observed a difference in
377 single voxel autocorrelation along the anterior-posterior and medial-lateral
378 hippocampal axes, where voxels with higher single voxel autocorrelation were
379 found in the anterior-medial hippocampus and voxels with lower single voxel
380 autocorrelation were found in the posterior-lateral hippocampus. Figure 5A
381 shows the group-level single voxel autocorrelation maps for the four navigation
382 conditions (as single voxel autocorrelation maps for lags 1-2 were similar, only
383 lag 1 is depicted in Figure 5A). The spatial distribution of single voxel
384 autocorrelation was similar across navigation conditions and was also similar to
385 the findings from Dataset 1. In the next section, we investigate the differences
386 between conditions in more depth.



388 **Figure 5. A) Single Voxel Autocorrelation: Lag 1.** Single voxel autocorrelation values
389 at lag 1 for every voxel in the hippocampus during spatial navigation. These values are
390 averaged across run and participant for each of the GPS, Familiar, Unfamiliar and
391 Mirrored conditions. A gradient from high to low autocorrelation is observed in the
392 anterior-posterior and medial-lateral axes, across all navigation conditions. **B)**
393 **Autocorrelation Clustering.** Cluster maps averaged across run and participant for each
394 route type. High single voxel autocorrelation voxels cluster in the anterior-medial
395 hippocampus and low single voxel autocorrelation voxels cluster in the posterior-lateral
396 hippocampus.

397

398 **Autocorrelation Clustering**

399 In order to determine clusters of single voxel autocorrelation within each
400 navigational condition, we repeated the autocorrelation clustering procedure
401 described above in Dataset 1 within the hippocampus. As with Dataset 1, this
402 revealed three distinct clusters in the left and right hemispheres for the Familiar,
403 Unfamiliar and Mirrored conditions (Figure 5B). For Familiar, Unfamiliar, and
404 Mirrored conditions, Cluster 1 was located in the anterior-medial HPC and had
405 the highest single voxel autocorrelation. Cluster 3 was located in the posterior-
406 lateral hippocampus and had the lowest single voxel autocorrelation. Cluster 2
407 was located between Cluster 1 and 3 and had intermediate single voxel
408 autocorrelation. The GPS condition had three clusters in the right hemisphere
409 and only two in the left.

410

411 **Relating single voxel autocorrelation to navigation condition**

412 Subjective difficulty ratings collected after each route (1 = difficult, 9 = easy)
413 suggested that across the navigation conditions, navigational difficulty increased.
414 Participants rated the GPS routes as the easiest ($M = 7.2$, $SD = 1.46$), followed

415 by the Familiar condition ($M = 6.98$, $SD = 2.05$), Unfamiliar condition ($M = 4.35$,
416 $SD = 2.66$), and the Mirrored condition, which was subjectively the most difficult
417 ($M = 3.97$, $SD = 2.42$).

418

419 As navigation becomes more difficult, it is beneficial to integrate or maintain
420 information over time, which may be reflected in changes in single voxel
421 autocorrelation. Specifically, more stable neural dynamics might enable
422 individuals to maintain information as one moves towards a goal. This prediction
423 leads to two possibilities. In the first, as navigational difficulty increases we might
424 observe a uniform change in single voxel autocorrelation across all voxels in the
425 hippocampus. A second possibility is that as difficulty increases, voxels that tend
426 to exhibit high autocorrelation during rest would differentially increase their
427 autocorrelation relative to voxels that tend to exhibit low autocorrelation. To
428 investigate these possibilities, we calculated the slope of the single voxel
429 autocorrelation (lag 1) along the anterior-posterior and medial-lateral axes. If
430 navigational difficulty leads to a uniform increase in autocorrelation, we would
431 observe no changes in the slope across these axes. However, if navigational
432 difficulty disproportionately affects the regions of the hippocampus that show high
433 autocorrelation during rest (Figure 2), then more difficult routes would elicit a
434 larger difference in autocorrelation values along the anterior-posterior and
435 medial-lateral axes, and therefore, a steeper slope. For easier routes, there
436 would be less difference in autocorrelation along the two axes, suggesting more
437 homogeneity of temporal dynamics along the axis and a shallower slope of
438 autocorrelation.

439

440 **Anterior-posterior HPC axis**

441 *Comparing single voxel autocorrelation slopes*

442 We compared autocorrelation slopes in the four route conditions: GPS, Familiar,
443 Unfamiliar, and Mirrored. For each participant, we averaged the single voxel
444 autocorrelation (lag 1) across all voxels on each 3mm slice of the hippocampus
445 (posterior-to-anterior direction) and calculated the slope coefficient across slices.
446 In both the left and right hemisphere, across all four navigation conditions, the
447 slope was positive, suggesting lower autocorrelation in the posterior
448 hippocampus and higher autocorrelation in the anterior hippocampus, which is
449 consistent with our findings from the clustering and single voxel autocorrelation
450 lag 1 analyses. Across participants, Mirrored runs had steepest slopes (*Left*: $M =$
451 0.79 , $SD = 0.60$; *Right*: $M = 0.55$, $SD = 0.80$) followed by Unfamiliar (*Left*: $M =$
452 0.69 , $SD = 0.53$; *Right*: $M = 0.41$, $SD = 0.40$), Familiar (*Left*: $M = 0.63$, $SD = 0.46$;
453 *Right*: $M = 0.31$, $SD = 0.25$), and GPS routes (*Left*: $M = 0.53$, $SD = 0.42$; *Right*: M
454 $= 0.21$, $SD = 0.28$).

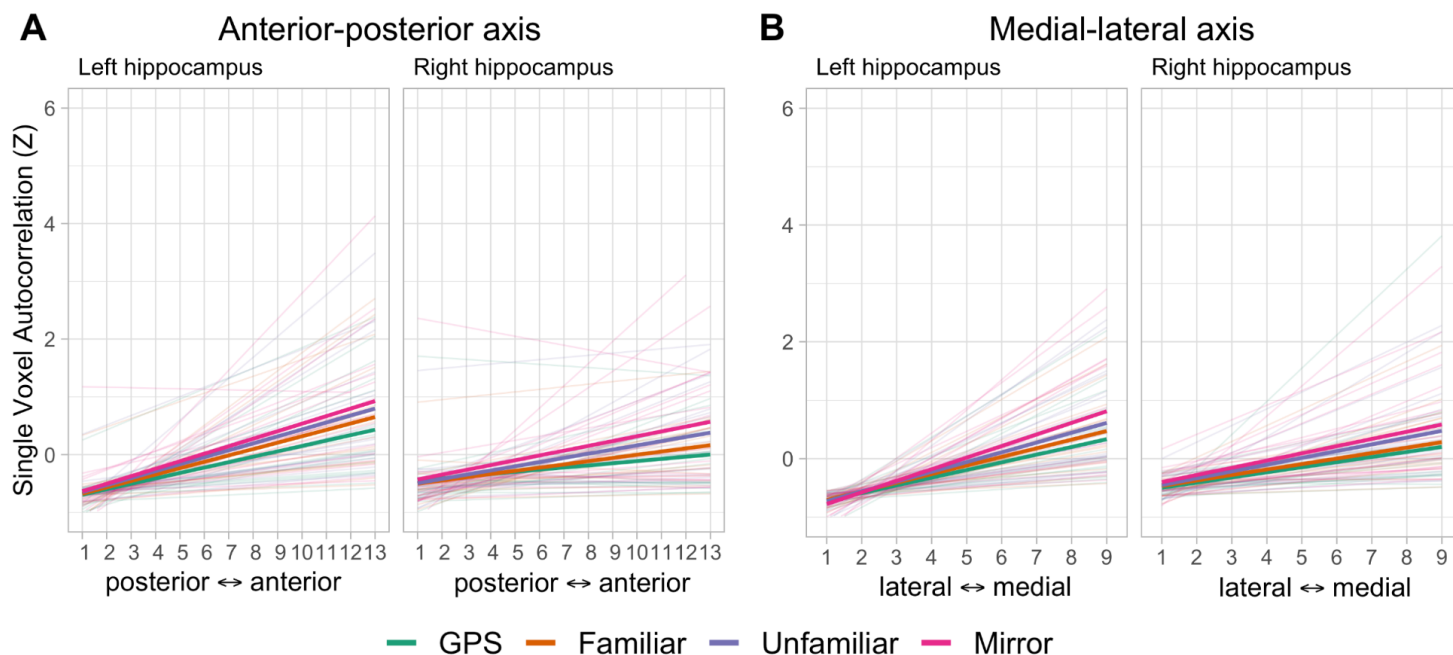
455

456 To test whether there was a significant difference between single voxel
457 autocorrelation during different navigation conditions, we ran a mixed effects
458 model on the single voxel autocorrelation slopes along the anterior-posterior axis.
459 We included hemisphere and condition (GPS, Familiar, Unfamiliar, and Mirrored)
460 as predictors in the model and participants as a random intercept in the random
461 effects term. We found a significant effect of hemisphere ($F(1, 481.99) = 42.22$, p
462 $< .001$) and a significant effect of navigation condition ($F(3, 483.04) = 6.92$, p
463 $< .001$) (Figure 6A). Their interaction was not significant.

464

465 A post hoc analysis of the main effect of hemisphere revealed that the single
466 voxel autocorrelation slope was greater in the left hippocampus compared to the
467 right hippocampus ($t(482) = 6.49$, $p < .001$). Pairwise comparisons of the different
468 navigational conditions (collapsed across hemisphere) revealed that single voxel
469 autocorrelation slopes were significantly greater for the Mirrored compared to
470 GPS ($t(484) = 3.88$, $p < .001$) and Familiar ($t(482) = 3.71$, $p < .01$). There was no
471 significant difference between Mirrored and Unfamiliar conditions. These results
472 suggest that, across hemispheres, the single voxel autocorrelation slopes along
473 the anterior-posterior axis were modulated by navigation difficulty: navigation
474 runs with a steeper gradient of autocorrelation were related to more difficult
475 navigation conditions. We compared the average single voxel autocorrelation at
476 the two posterior-most and two anterior-most slices and found that single voxel
477 autocorrelation was higher in the anterior hippocampus compared to the
478 posterior hippocampus in both the left and right hemisphere (Left: anterior $>$
479 posterior $t(1998) = 22.23$, $p < .001$; Right: anterior $>$ posterior $t(1998) = 13.49$, p
480 $< .001$). This finding suggests that increases in the autocorrelation slope along
481 the anterior-posterior axis across conditions were driven by an increase in the
482 anterior hippocampus.

483



485 **Figure 5. Effect of navigational condition on single voxel autocorrelation slopes.**
 486 Average single voxel autocorrelation per slice along the anterior-posterior and medial-
 487 lateral axes for each navigation condition. **A) Anterior-posterior axis.** The left
 488 hippocampus had greater single voxel autocorrelation slopes compared to the right
 489 hippocampus. Across both hemispheres, slope along the anterior-posterior axis was
 490 modulated by navigational condition. The slope was greatest when participants
 491 navigated difficult routes (Mirrored and Unfamiliar routes) compared to easy routes (GPS
 492 and Familiar routes) **B) Medial-lateral axis.** The left hippocampus had greater single
 493 voxel autocorrelation slopes compared to the right hippocampus. Across both
 494 hemispheres, slope along the medial-lateral axis was modulated by navigational
 495 condition. The slope was greatest when participants navigated Mirrored routes
 496 compared to GPS, Familiar, and Unfamiliar routes. Bold lines represent the group
 497 average across all participants, faded lines represent each participant.

498 **Medial-lateral HPC axis**

499 *Comparing single voxel autocorrelation slopes*

500 For each participant, we averaged the single voxel autocorrelation (lag 1) across
 501 all voxels on each 3mm slice of the hippocampus (lateral-to-medial direction) and
 502 calculated the slope coefficient across slices. In both the left and right
 503 hemisphere, across all four navigation conditions, the slope was positive,
 504 suggesting lower autocorrelation in the lateral hippocampus and higher
 505 autocorrelation in the medial hippocampus. This observation is consistent with
 506 our findings from the clustering and single voxel autocorrelation lag 1 analyses.
 507 Across participants, Mirrored runs had steepest slopes (*Left*: $M = 1.63$, $SD =$
 508 1.15 ; *Right*: $M = 1.45$, $SD = 1.77$) followed by Unfamiliar (*Left*: $M = 1.37$, $SD =$
 509 1.15 ; *Right*: $M = 1.45$, $SD = 1.77$)

510 0.95; *Right*: $M = 1.13$, $SD = 1.20$), Familiar (*Left*: $M = 1.21$, $SD = 0.74$; *Right*: $M =$
511 0.92 , $SD = 0.98$), and GPS routes (*Left*: $M = 1.08$, $SD = 0.80$; *Right*: $M = 0.89$, SD
512 $= 1.45$).

513

514 We ran a mixed effects model on the single voxel autocorrelation slopes along
515 the medial-lateral axis with hemisphere and condition as predictors and
516 participant as a random intercept in the random effects term. We found a
517 significant effect of hemisphere ($F(1, 482.03) = 5.03$, $p < .05$) and a significant
518 effect of navigation condition ($F(3, 482.71) = 7.10$, $p < .001$) (Figure 6B). Their
519 interaction was not significant.

520

521 A post hoc analysis of the main effect of hemisphere revealed that the single
522 voxel autocorrelation slopes were greater in the left than the right hippocampus
523 ($t(482) = 2.24$, $p < 0.05$). Pairwise comparisons of the different navigational
524 conditions (collapsed across hemisphere) revealed that single voxel
525 autocorrelation slopes were significantly greater for the Mirrored compared to
526 GPS ($t(483) = 3.42$, $p < .01$), greater for Mirrored compared to Familiar ($t(482) =$
527 4.18 , $p < .001$), and greater for Mirrored compared to Unfamiliar ($t(482) = 2.61$, p
528 $< .05$). These results suggest that, across hemispheres, the single voxel
529 autocorrelation slopes along the medial-lateral axis were modulated by
530 navigation difficulty: navigation runs that had a steeper gradient of
531 autocorrelation were related to more difficult navigation conditions. We compared
532 the average single voxel autocorrelation at the two medial-most and two lateral-
533 most slices and found that single voxel autocorrelation was higher in the medial
534 hippocampus than the lateral hippocampus in both the left and right hemisphere
535 (*Left*: medial > lateral $t(1998) = 17.76$, $p < .001$; *Right*: medial > lateral $t(1998) =$
536 14.91 , $p < .001$). This suggests that increases in the autocorrelation slope along
537 the medial-lateral axis across conditions is driven by an increase in the medial
538 hippocampus.

539

540 **Discussion**

541

542 Here we present a novel autocorrelation measure to investigate intra-
543 hippocampal and intra-entorhinal processing. We provide the first evidence of a
544 medial-lateral gradient of autocorrelation in the hippocampus, as well as a
545 posterior-medial and anterior-lateral gradient in the ERC. We found that voxels in
546 the anterior-medial hippocampus have a highly correlated, slower changing
547 signal, whereas voxels in the posterior-lateral hippocampus have a less
548 correlated, faster changing signal (Figure 2) (Brunec, Bellana, et al., 2018; Raut
549 et al., 2020). Our study highlights the importance of examining the medial-lateral

550 axis of the hippocampus, which has previously been an under-studied feature of
551 hippocampal organization. We find novel evidence for a continuous gradient in
552 the ERC, with greater autocorrelation in the posteromedial ERC and lower
553 autocorrelation in the anterolateral ERC (Figure 4). Lastly, the present study is
554 the first to show that gradients of single voxel autocorrelation in the hippocampus
555 are related to behavior during navigation. Specifically, autocorrelation gradients
556 in the anterior-posterior and medial-lateral axes, as measured by the slope,
557 increased for difficult routes and were steepest in the left hemisphere (Figure 6).
558 This increase in slope was driven by increases in the anterior-medial
559 hippocampus.

560
561 Our data-driven approach — which allows voxels to cluster according to their
562 single voxel autocorrelation, uncovered a multidimensional gradient in both the
563 anterior-posterior and medial-lateral axes in both the hippocampus and ERC
564 (Figure 2 & 4). In the hippocampus, the anterior-posterior axis has been studied
565 with respect to its role in representing graded information, for example coarse-
566 grained to fine-grained information (Poppenk et al. 2013; Strange et al., 2014),
567 large to small spatial distances (Evensmoen et al., 2013; Nielson et al., 2015;
568 Peer et al., 2019;) and long to short temporal distance (Bellmund et al., 2019;
569 Nielson et al., 2015). Investigations of representational differences along the
570 medial-lateral axis, however, have been limited because prior work has used
571 predefined anatomical segmentations limited to the anterior and posterior
572 portions of the long axis of the hippocampus. Our single voxel autocorrelation
573 method is not restricted by predefined ROIs and proves to be a more precise
574 measure that detects subtle differences in signal along the medial-lateral axis
575 that have been previously overlooked and that are modulated by navigational
576 difficulty. In addition to the hippocampus, we found similar distinctions in the
577 ERC. We observed a gradient of single voxel autocorrelation organization, such
578 that greater single voxel autocorrelation was observed in the posterior-medial
579 region and lower single voxel autocorrelation in the anterolateral region of the
580 ERC (Figure 4). This gradient is consistent with previous neuroimaging
581 investigations of ERC which used high-resolution fMRI and functional
582 connectivity to define distinct subregions within the human ERC (Maass et al.,
583 2015; Navarro Schröder et al., 2015). Our analytic technique, however, goes
584 beyond this prior work by demonstrating, for the first time, continuous gradients
585 of autocorrelation in the ERC.

586
587 The present study demonstrates that the autocorrelation of the fMRI signal is not
588 just global noise, but instead carries meaningful information about brain function
589 that is directly related to behavior. Autocorrelation is frequently characterized as

590 noise that masks meaningful signals and is unrelated to cognition, but recent
591 research suggests that autocorrelation might be a global organizing principle and
592 reflects intrinsic functional hierarchies in the brain (Irish & Vatansever, 2020;
593 Raut et al., 2020). For example, an analysis of resting state fMRI data calculated
594 the autocorrelation decay in single voxels across a temporal window (0-8
595 seconds) and found a significant large-to-small timescale gradient along the
596 anterior-posterior axis in the hippocampus (Raut et al., 2020), which is consistent
597 with reports by Brunec, Bellana, et al. (2018). Recent research has also linked
598 autocorrelation with global differences in cognitive state (task vs. rest) and
599 mental state (healthy vs. schizophrenia) (Arbabshirani et al., 2019). While this
600 study cannot address the direct link between the autocorrelation gradients and
601 behavior, this work suggests that autocorrelation can be used to discriminate
602 between cognitive states that are uniform across the brain, leaving open the
603 question of how autocorrelation gradients in specific brain regions might be
604 related to differences in cognition during a behavioral task. Our analysis
605 technique demonstrated novel gradients during resting state, and can also be
606 applied to task related activation to reveal their relation to on-going behavior and
607 is the first to show that changes in single voxel autocorrelation gradients are
608 directly related to changes in difficulty during a navigation task.

609
610 Anterior hippocampal voxels are more stable across time compared to the
611 posterior hippocampus, which might enable the anterior hippocampus to maintain
612 prior information across time during goal-directed navigation (Brunec, Bellana, et
613 al., 2018). Our method proved to be a more sensitive measure than previous
614 techniques (e.g., Brunec, Bellana et al., 2018) because we were able to show
615 differences in autocorrelation across navigation conditions. More specifically we
616 found that the autocorrelation in the anterior-medial hippocampus increased
617 during navigation of difficult routes (Figure 6). The autocorrelation signal may
618 reflect the mechanism by which the hippocampus holds onto the past and carries
619 it forward during navigation when we are in unfamiliar or unpredictable
620 environments. For example, when navigating an unfamiliar route to a distant
621 goal, the local details of the environment might not be helpful to orient oneself in
622 relation to the goal; it may be more efficient, therefore, to keep in mind a coarser,
623 overall map of the environment with information about steps already taken in
624 order to reach the goal destination successfully. This large-scale representation
625 may not be as useful to keep online during navigation of well-known or familiar
626 routes where local details are sufficient for orienting and navigating to the goal,
627 which could explain the decreased single voxel autocorrelation in the signal
628 throughout the familiar routes (Figure 6). This hypothesis is supported by
629 previous research which has shown that the anterior hippocampus plays an

630 important role in representing larger spatial and temporal distances (Evensmoen
631 et al., 2013; Nielson et al., 2015) as well as representing coarser-grained, global
632 representations (Collin et al., 2015).

633

634 We found that both of the single voxel autocorrelation gradients (anterior-
635 posterior and medial-lateral) were steeper in the left hemisphere compared to the
636 right. It is still unclear whether this is representative of a stable difference in
637 autocorrelation between the hemispheres or whether this reflects different types
638 of information that are engaged across the two hemispheres during navigation.
639 Future research is needed to determine the nature of this hemispheric difference.

640

641 Another non-mutually exclusive possibility is that the single voxel autocorrelation
642 is representative of predictions that are cast into the future. The notion that
643 increased temporal similarity is indicative of an extended spatiotemporal
644 representation is supported by recent work investigating the predictive horizons
645 along the hippocampal anteroposterior axis during navigation (Bruenc &
646 Momennejad, 2019). Brunec and Momennejad (2019) found that as participants
647 virtually navigated familiar, real-world routes (a subset of the familiar routes
648 presented here), hippocampal activity was related to a hierarchical scale of
649 horizon representations, in which the posterior hippocampus represented steps
650 closer in the future trajectory (~25m) while the anterior hippocampus represented
651 steps further in the future trajectory (~175m). It is possible, therefore, that the
652 single voxel autocorrelation we observed helps represent an upcoming
653 navigational trajectory, with immediate goals represented in posterior-lateral
654 regions and more distal goals in the anterior-medial hippocampus. The predictive
655 role of the hippocampus has also been observed in perception, particularly when
656 the stimulus was visually complex (Kok et al., 2020). Our method and findings
657 open the door for future studies using high resolution neuroimaging in
658 combination with a task that parametrically modulates the amount of information
659 that is carried over time in both predictable (familiar) and unpredictable
660 (unfamiliar) environments to uncover content that is carried forward via the
661 autocorrelation signal.

662

663 Although we were not able to relate the autocorrelation in ERC to behavior due to
664 the resolution of the navigation data, if we apply the same logic we used for the
665 hippocampus, our findings are consistent with the notion that aERC codes for
666 local details and perceptual aspects of experience, whereas the pmERC codes
667 for global contexts. Specifically, the (antero-)lateral ERC has been linked to fine-
668 grained temporal processing (Montchal et al., 2019; Tsao et al., 2018) and to
669 processing of object-context and within-object details (Yeung et al., 2017; 2019).

670 The low autocorrelation we observed in the aERC might indicate faster updating
671 of moment-to-moment changes and therefore support fine-grained
672 representations. Future investigations can use our method to analyze continuous
673 changes along both anterior-posterior and medial-lateral axes of the ERC without
674 being restricted to anatomical subfield segmentations, perhaps revealing a more
675 nuanced understanding of the organization of the ERC. We observed two
676 consistent clusters in the left hemisphere and three consistent clusters in the
677 right hemisphere, which suggests that in this dataset there was more variability in
678 the left ERC intermediate cluster. Future research is needed to determine
679 whether this is a stable property of the temporal organization of the left ERC that
680 can be replicated across other datasets.

681
682 It is currently unclear how the posterior-medial and anterior-lateral subregions of
683 the ERC are functionally related to the anterior and posterior regions of the
684 hippocampus. In the present study we found that clusters in the anterior-medial
685 hippocampus and posterior-medial ERC had high single voxel autocorrelation,
686 whereas clusters in the posterior-lateral hippocampus and antero-lateral ERC
687 had low single voxel autocorrelation. These distinctions along the anterior-
688 posterior and medial-lateral axes of the ERC are consistent with previous
689 functional connectivity findings (Navarro Schröder et al., 2015), however
690 functional connectivity and neuroanatomical studies in humans have been limited
691 and do not find any clear differences between the anterior and posterior portions
692 of the hippocampus with respect to their connectivity to different subregions in
693 the ERC (Maass et al., 2015; Navarro Schröder et al., 2015). Functional
694 connections between these regions might be evident in the scale of information
695 processing in the hippocampus and ERC. For example, it is possible that the
696 pattern of low single voxel autocorrelation in anterior-lateral ERC and posterior-
697 lateral hippocampus supports fine-grained processing — precise temporal
698 processing in the anterior-lateral ERC (Bellmund et al., 2019; Montchal et al.,
699 2019) and local spatial details in the posterior hippocampus (Doeller et al., 2008;
700 Evensmoen et al., 2013; Hirshhorn et al. 2012; Lee et al., 2012).

701
702 There are currently no clear neuroanatomical links between the anterior-lateral
703 ERC and posterior-lateral hippocampus or the anterior-medial hippocampus and
704 posterior-medial ERC. There are, however, probable connections between the
705 anterior ERC and lateral hippocampus and posterior ERC with medial
706 hippocampus (Strange et al., 2014; Witter & Amaral 2020; Nilssen et al., 2019;
707 Witter et al., 2017). Our results, therefore, open the door for future investigations
708 to characterize more fully the nature of anterior and posterior hippocampal signal
709 dynamics in relation to the entorhinal subregions in humans and in relation to

710 other structures, such as prefrontal cortex (Barredo et al., 2015; Vaidya & Badre,
711 2020).

712

713 The results presented here reveal, for the first time, two continuous gradients
714 along the anterior-posterior and medial-lateral axes in the hippocampus and
715 ERC. One outstanding question is whether there is new information that can be
716 gained by investigating the two autocorrelation gradients separately, or whether
717 the information they represent is redundant. For example, do tasks that evoke a
718 steep autocorrelation gradient along the anterior-posterior axis necessarily evoke
719 a similarly steep gradient along the medial-lateral axis or are there tasks in which
720 these two gradients act in opposing directions (e.g., change in anterior-posterior
721 slope but no change or change in opposite direction in medial-lateral slope).
722 Another outstanding question is whether our novel single voxel autocorrelation
723 method can be applied with shorter timescales so that they can be used with
724 event-related designs. Here we use the entire timecourse of the voxel's activity to
725 calculate the single voxel autocorrelation throughout the entire run, but it remains
726 to be seen whether we can adapt our method to examine how autocorrelation
727 changes over shorter time windows. This would allow us to ask new questions
728 about what kind of information is being carried in the autocorrelation signal during
729 discrete or shorter events and at event boundaries, which are known to trigger
730 changes in hippocampal activity associated with integration of information across
731 events (Dubrow & Davachi, 2013; Ezzyat & Davachi, 2014). Finally, this method
732 can be used to investigate differences in autocorrelation within subfields of the
733 hippocampus. For example, it has been proposed that CA1 is implicated in
734 integrating information in memory, whereas DG/CA3 which mediates pattern
735 separation may be more implicated in making fine distinctions in memory (Kyle et
736 al., 2015; Leutgeb et al., 2004; Schapiro et al., 2017; Yassa & Stark, 2011).
737 Integration processes in CA1, therefore, might be supported by voxels with high
738 single voxel autocorrelation while separation processes in DG/CA3 might be
739 better supported by low single voxel autocorrelation. Future research using our
740 method and high-resolution fMRI is needed to test these differences within
741 subfields.

742

743 Our studies were inspired initially by single-unit recording studies in rodents
744 (Brun et al., 2008; Cavanagh et al., 2016; Gothard et al., 1996; Kjelstrup et al.,
745 2008; Maurer et al., 2005). We believe our findings, however, have gone beyond
746 replicating the rodent findings in humans, a worthy task in its own right, but
747 extended the findings to the point that they can now be used to inform future
748 studies in rodents and humans. We provide some examples in which this is the
749 case. For example, our method enabled us to find differences in autocorrelation

750 along the anterior-posterior and medial-lateral axes in the entorhinal cortex,
751 which have only been examined in a restricted region in rodents (Brun et al.,
752 2008). Our findings are consistent with neuroanatomical and neurophysiological
753 divisions in that structure (human: Maass et al., 2015; monkey: Witter & Amaral,
754 2021; rat: Witter et al., 2017). Second, although activity of a single voxel,
755 comprised of thousands of neurons, may be considered to be a coarser unit of
756 analysis than recordings from single units, it may be the case that it is the
757 operation of a population of these neurons that is most closely linked to
758 organizational temporal dynamics. It is the gradients revealed by autocorrelation
759 at the single voxel level that enabled us to link hippocampal dynamics to
760 behavior. In addition, we were able to segment the populations into clusters,
761 suggesting subdivisions that would not be evident at the single-unit level. It would
762 be worthwhile to determine whether similar clusters are found in rodents and
763 examine their functional significance. Similar analyses at the population-level in
764 rodents may yield information about the relation of neural dynamics to higher-
765 level memory representations and goals, an enterprise that is just beginning
766 (Jacob & Josselyn, 2020; Morrissey et al., 2017).

767

768 Our results provide compelling evidence for a gradation of single voxel
769 autocorrelation in the hippocampus and ERC. As predicted, our single voxel
770 method proved to be a fine-grained measure that revealed subtleties in the
771 spatial organization of autocorrelation, going beyond prior methods, and allowed
772 us to observe graded signals along anterior-posterior and medial-lateral axes in
773 both regions. Further, we show for the first time that differences in single voxel
774 autocorrelation gradients in the hippocampus can be directly related to
775 differences in difficulty during a virtual navigation task, thus opening the door for
776 future research to ask new questions of the autocorrelation signal and uncover
777 how it is related to behavior.

778

779 **Materials and Methods**

780

781 **Dataset 1: Resting state fMRI**

782 ***Participants***

783 We analyzed resting state fMRI data from 44 participants (14 male) from the
784 Human Connectome Project (HCP) Retest dataset. This dataset consists of data
785 from 44 participants who were scanned twice using the full HCP imaging
786 protocol. All subject recruitment procedures and informed consent forms,
787 including consent to share de-identified data, were approved by the Washington
788 University Institutional Review Board (IRB) (Glasser et al. 2016). The present
789 analysis of this dataset was approved by the University of Toronto research

790 ethics board.

791

792 ***Scanning parameters and preprocessing***

793 Resting state data were collected using a multiband EPI pulse sequence (TR =
794 720 ms, TE = 33.1 ms, 72 slices with 2 mm thickness, FOV = 208 x 180 mm,
795 voxel size = 2x2 mm, Flip angle = 52, Multiband factor = 8, Scan time = 14
796 minutes and 33 seconds). Each run was repeated twice, with a left-to-right and a
797 right-to-left phase encoding direction. The presented results are generated from
798 data with the left-to-right phase encoding direction.

799

800 Initial fMRI preprocessing steps already applied to the downloaded data included
801 fieldmap correction, motion correction, brain extraction, registration to standard
802 space, and intensity normalization (Glasser et al., 2013; Smith et al., 2013; Van
803 Essen et al., 2013). The data were further preprocessed using the FIX tool in
804 FSL (Griffanti et al., 2014; Salimi-Khorshidi et al., 2014), and noise components
805 related to head motion and other artifacts were removed. To eliminate high
806 frequency noise and artifacts, fMRI signals are low-pass filtered using MATLAB
807 IIR Butterworth filter (designfilt function in Signal Processing Toolbox) with cutoff
808 frequency of 0.1 Hz.

809

810 ***Single voxel autocorrelation method***

811 *Computing single voxel autocorrelation*

812 Bilateral hippocampal and entorhinal masks were generated using the Harvard-
813 Oxford Atlas in FSL. For each voxel inside each of the regions of interest (ROIs),
814 unbiased autocorrelation (as implemented in MATLAB xcorr function) was
815 calculated. Specifically, the timecourse of a single voxel's activity was correlated
816 with itself shifted by a temporal lag, the length of 1 TR (Dataset 1 TR = 720 ms).
817 We repeated this process, shifting the timecourse forward by 1 lag (720 ms) and
818 correlating it with the original, non-shifted timecourse until a maximum temporal
819 shift of 4 seconds was reached. We chose 4 seconds because it has been shown
820 that the autocorrelation of the fMRI signal in the gray matter drops off after 4
821 seconds (i.e., it is not distinguishable from the autocorrelation of other noise)
822 (Bollmann et al., 2018). For example, the non-shifted timecourse was correlated
823 with lag 1 (length of 1 TR), lag2 (length of 2 TRs), etc. (Figure 1). The
824 autocorrelation (AC) computed for each lag was stored in a vector. The
825 autocorrelation vector (single voxel autocorrelation vector) contained 5 values
826 (one single voxel autocorrelation for each lag). This approach resulted in a single
827 voxel autocorrelation vector for each voxel (Figure 1A). All single voxel
828 autocorrelation values were normalized by subtracting the mean and dividing by
829 the standard deviation within each mask so that meaningful comparisons could

830 be made between the two fMRI datasets (resting state and task). Single voxel
831 autocorrelation maps were then averaged across the first and second runs from
832 the 44 participants to generate an average overall map (e.g., Figure 1B).

833

834 *Single voxel autocorrelation – Reliability Analysis*

835 To verify that the observed single voxel autocorrelation pattern was not a
836 measurement artifact (e.g., head motion, magnetic field inhomogeneity,
837 physiological artifacts, etc.), we tested the reliability of the single voxel
838 autocorrelation pattern within an individual. In our case, the single voxel
839 autocorrelation pattern was deemed reliable if there was a high degree of
840 agreement between the single voxel autocorrelation values generated from
841 different runs from the same participant compared to runs from different
842 participants. Reliability of the single voxel autocorrelation values was measured
843 by calculating the Euclidean distance (ED) between the single voxel
844 autocorrelation vectors for all pairs of run-wise datasets. 44 participants with 2
845 repeated sessions produced 44 intra-subject and 3784 inter-subject ED values.
846 The lower the ED between two single voxel autocorrelation vectors, the higher
847 the similarity between them. We expected to see more similar single voxel
848 autocorrelation patterns between single voxel autocorrelation vectors generated
849 from two runs of the same participant compared to two runs from different
850 participants (lower intra-subject ED compared to inter-subject ED). The inter-
851 subject and intra-subject ED are not completely independent from one another,
852 therefore we used nonparametric permutation to test for significance. We
853 randomly shuffled the intra- and inter-subject labels and pulled two samples of
854 size 44 (intra-subject) and 3784 (inter-subject). We calculated the mean
855 difference between the two samples and repeated this process 10,000 times,
856 resulting in a histogram of mean differences under the null hypothesis (i.e., the
857 difference between intra- and inter-subject ED equal to zero). We compared the
858 observed difference between intra- and inter-subject EDs with the null distribution
859 and calculated nonparametric p-values. Permutation tests were conducted using
860 a permutation testing package in Matlab (Laurens, 2021).

861

862 *Computing single voxel autocorrelation clusters (Autocorrelation Clustering)*

863 The Euclidean distance between the single voxel autocorrelation vectors of each
864 voxel pair in each mask was calculated to create a distance matrix. The distance
865 matrix was first normalized (i.e., divided by the maximum value) and then
866 subtracted from 1 to generate a similarity matrix ranging from 0 to 1. This
867 similarity matrix was used to generate hippocampal clusters using the modularity
868 optimization algorithm proposed by (Blondel et al., 2008; Wickramarachchi et
869 al., 2014). Unlike the majority of the clustering methods, modularity optimization

870 does not require to assign the number of clusters and estimates the optimum
871 number of clusters from data. In addition to clustering at the level of each
872 individual, group-level clustering was performed by averaging the similarity
873 matrices of all participants (e.g., Figure 1C).

874

875 *Autocorrelation Clustering – Reliability Analysis*

876 Reliability of the clustering was measured by calculating the overlap between the
877 generated clusters using the Jaccard coefficient. The Jaccard coefficient of
878 regions A and B is defined as:

879

$$880 \quad J(A, B) = \frac{|A \cap B|}{|A \cup B|}$$

881

882 Where $|A \cap B|$ is the number of common voxels in both A and B (intersection)
883 and $|A \cup B|$ is the number of voxels in A and B combined (union). Individual
884 parcellations were then compared to the group-level parcellation to examine the
885 consistency of parcellation. The Jaccard coefficient was calculated both intra-
886 subject (overlap between clusters extracted from two runs from the n th subject)
887 and inter-subject (overlap between the cluster from the n th subject and the same
888 cluster estimated in all other subjects).

889

890 Assuming that the single voxel autocorrelation pattern is consistent across the
891 two runs of the same participant, we expected there to be greater spatial overlap
892 (higher Jaccard coefficient) among clusters within an individual compared to
893 between different individuals. The Jaccard coefficients for clusters within
894 participants are not completely independent from the Jaccard coefficients for
895 clusters between participants, therefore we used nonparametric permutation to
896 test for significance. For each cluster, we randomly shuffled the intra- and inter-
897 subject labels and pulled two samples of size 44 (intra-subject) and 3784 (inter-
898 subject). We calculated the mean difference between the two samples and
899 repeated this process 10,000 times, resulting in a histogram of the mean
900 differences under the null hypothesis (i.e., the difference between intra- and -
901 inter-subject Jaccard coefficient equal to zero). We compared the observed
902 difference between intra- and inter-subject Jaccard coefficients with the null
903 distribution and calculated nonparametric P values.

904

905 **Dataset 2: Navigation fMRI**

906 *Participants*

907 Task fMRI data is from Brunec, Bellana, et al. (2018), where 19 participants (9
908 males; mean age 22.58 years, range 19-30 years) were scanned while
909 navigating Google Street View routes around the city of Toronto. All subject

910 recruitment procedures and informed consent was approved by the University of
911 Toronto research ethics board.

912

913 ***Paradigm***

914 Participants met with the experimenter ahead of time and built routes that were
915 either highly familiar or less familiar to them (e.g., frequently travelled or not).
916 Participants then returned to the lab for their second session and were scanned
917 while they navigated four different types of routes. 1) Familiar: participants
918 started at a familiar landmark and navigated to a familiar goal destination via a
919 familiar route, 2) Mirrored: participants started at a familiar landmark and
920 travelled to a familiar destination via a familiar route, but the images of the route
921 were mirrored (left-right reversed), 3) Unfamiliar: participants started at a familiar
922 location, navigated to a familiar destination, but they were instructed to take an
923 unfamiliar route between the two, and 4) GPS: participants started at an
924 unfamiliar location in an unfamiliar part of town and pressed arrow keys following
925 the directions displayed by an arrow on the screen to the goal destination.
926 Participants completed four unique routes in each condition, sixteen routes in
927 total (1 route = 1 scanned run). At the end of each route, participants rated the
928 difficulty of the route on a scale from 1 (difficult) to 9 (easy).

929

930 ***Scanning parameters and preprocessing***

931 Participants were scanned with a 3T Siemens MRI scanner at Baycrest's Rotman
932 Research Institute. A high-resolution 3D MPRAGE T1-weighted pulse sequence
933 image (160 axial slices, 1 mm thick, FOV = 256 mm) was first obtained to register
934 functional maps against brain anatomy. Functional imaging was performed to
935 measure brain activation by means of the blood oxygenation level dependent
936 (BOLD) effect. Functional T2*-weighted images were acquired using echo-planar
937 imaging (30 axial slices, 5 mm thick, TR = 2000 ms, TE = 30 ms, flip angle = 70
938 degrees, FOV = 200 mm). The native EPI resolution was 64 x 64 with a voxel
939 size of 3.5mm x 3.5mm x 5.0mm. Images were first corrected for head motion
940 using the Analysis of Functional NeuroImages (AFNI; Cox, 1996). All subsequent
941 analysis steps were conducted using the statistical parametric mapping software
942 SPM12.

943

944 Preprocessing involved slice timing correction, spatial realignment and co-
945 registration, with a resampled voxel size of 3mm isotropic, with no spatial
946 smoothing. As all of our analyses rely on covariance, we additionally regressed
947 out the mean time-courses from participant-specific white matter, and
948 cerebrospinal fluid masks, alongside estimates of the 6 rigid body motion
949 parameters from each EPI run. To further correct for the effects of motion which

950 may persist despite standard processing (Power et al., 2012), an additional
951 motion scrubbing procedure was added to the end of our preprocessing pipeline.
952 Using a conservative multivariate technique, time points that were outliers in both
953 the six rigid-body motion parameter estimates and BOLD signal were removed,
954 and outlying BOLD signal was replaced by interpolating across neighboring data
955 points. Motion scrubbing further minimizes any effects of motion-induced spikes
956 on the BOLD signal, over and beyond standard motion regression, without
957 leaving sharp discontinuities due to the removal of outlier volumes (for details,
958 see Campbell et al., 2013). To enable comparisons at the group-level, the final
959 step of the preprocessing involved warping participants' functional data to the
960 MNI-space template.

961

962 ***Single voxel autocorrelation method***

963 *Computing single voxel autocorrelation*

964 To compute the single voxel autocorrelation, we completed the same procedure
965 outlined in Dataset 1. We used the same bilateral hippocampal masks to extract
966 the HPC voxels in Dataset 2. For each voxel, the single voxel autocorrelation
967 was calculated by repeatedly shifting temporal lags (length of 1 TR) until a
968 maximum lag of 4 seconds was reached. In Dataset 2 the TR was 2000 ms;
969 therefore, single voxel autocorrelation for 2 lags (or 2 TRs) was calculated,
970 resulting in a maximum lag of 4 seconds. As outlined in the procedure above,
971 single voxel autocorrelation values were normalized by subtracting the mean and
972 dividing by the standard deviation. Single voxel autocorrelation was calculated for
973 all four runs of each navigational condition (Familiar, Unfamiliar, Mirrored, GPS).
974 The single voxel autocorrelation was averaged across the four scanned runs
975 (unique routes), resulting in four different maps (one for each navigational
976 condition). Single voxel autocorrelation maps were then averaged across the 19
977 participants to generate an average group map for each navigation condition.

978

979 Participants completed 16 navigation runs (four in each condition) at their own
980 pace. Because the conditions varied in difficulty, the average number of TRs
981 differed across conditions and participants. Every route was 2-10 km long and
982 the average run (route) length was 137.6 TRs (2 s TRs). The average number of
983 TRs was lowest in the GPS condition ($M = 92.13$, $SD = 17.44$), followed by the
984 Familiar condition ($M = 136.45$, $SD = 39.18$), the Mirrored condition ($M = 155.73$,
985 $SD = 36.84$), and the Unfamiliar condition ($M = 158.78$, $SD = 32.13$). In order to
986 compare single voxel autocorrelation across scanned runs with a similar number
987 of TRs/lengths, we chose to filter out any runs that were unusually short (that the
988 participant either didn't complete or completed very quickly). We excluded runs
989 that were less than 88 TRs long. This resulted in an average of 13.36 runs ($SD =$

990 1.21) per participant. The GPS runs were disproportionately shorter than the
991 other conditions, resulting in more GPS runs excluded than other conditions. The
992 average number of routes included in the following analyses per participant are
993 as follows: Mirrored (M=3.89, SD=0.31), Unfamiliar (M=3.84, SD=0.50), Familiar
994 (M=3.68, SD=0.47), GPS (M=1.95, SD=1.22).

995

996 *Computing autocorrelation clusters (Autocorrelation Clustering)*

997 We repeated the single voxel autocorrelation clustering procedure described
998 above in Dataset 1 to determine clusters of single voxel autocorrelation within
999 each navigational condition.

1000

1001 ***Relating single voxel autocorrelation to navigation condition***

1002 *Calculating single voxel autocorrelation slopes*

1003 To investigate how the spatial distribution of single voxel autocorrelation is
1004 related to navigation difficulty, we compared the single voxel autocorrelation (lag
1005 1) slopes across the four different conditions: GPS, Familiar, Unfamiliar, and
1006 Mirrored. First, for each participant, we extracted the single voxel autocorrelation
1007 (lag 1) from every voxel. We averaged the single voxel autocorrelation across all
1008 voxels on each slice of the hippocampus. We used 3 mm slices in the anterior-
1009 posterior direction (Y-direction), resulting in thirteen slices. Using a linear
1010 regression, we calculated the slope coefficient for the single voxel autocorrelation
1011 across slices for each navigation run. We then repeated the same procedure,
1012 using 3 mm slices in the medial-lateral direction (X-direction), resulting in 9
1013 slices. We computed the slopes and compared them across navigation
1014 conditions and hemispheres.

1015

1016 To test whether there was a significant difference between single voxel
1017 autocorrelation during different navigation conditions, we ran a mixed effects
1018 model on the single voxel autocorrelation slopes along the anterior-posterior and
1019 medial-lateral axes. This analysis was conducted in R (R Core Team, 2019)
1020 using the afex (Singmann et al., 2020) and the tidyverse packages (Wickham,
1021 2017).

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