AUTOMATED OPTIMIZATION OF RESIDUAL REDUCTION ALGORITHM PARAMETERS IN OPENSIM

Jordan T. Sturdy[1], Anne K. Silverman[1], Nathan T. Pickle[1,2]

[1] Colorado School of Mines, Golden, CO
[2] CFD Research Corp., Huntsville, AL

Word count: Abstract (133), Paper (2270)

Keywords: Biomechanics, Dynamic Consistency, OpenSim, RRA, MATLAB, Python, movement simulation

Abstract

The residual reduction algorithm (RRA) in OpenSim is designed to improve dynamic consistency of kinematics and ground reaction

forces in movement simulations of musculoskeletal models. RRA requires the user to select numerous tracking weights for the joint

kinematics to reduce residual errors. Selection is often performed manually, which can be time-consuming and is unlikely to yield

optimal tracking weights. A multi-heuristic optimization algorithm was used to expedite tracking weight decision making to reduce

residual errors. This method produced more rigorous results than manual iterations and although the total computation time was not

significantly reduced, this method does not require the user to monitor the algorithm's progress to find a solution, thereby reducing

manual tuning. Supporting documentation and code to implement this optimization is freely provided to assist the community with

developing movement simulations.

1. INTRODUCTION

Musculoskeletal models and simulations have seen significant increase in adoption in recent years, facilitated by software platforms

such as OpenSim (Delp et al., 2007, simtk.org). Inverse dynamics calculations are frequently the basis of these simulations. Inverse

dynamics uses experimental observations, i.e., ground reaction forces and joint kinematics, to calculate the joint moments required to

produce these observed data (Yamaguchi, 2005). This calculation contains multiple sources of error including modeling assumptions

(e.g., rigid body assumptions, segment inertial properties), and measurement error (e.g., soft tissue artifact). These sources of error result

in dynamic inconsistency (Kingma and Toussaint, 1996; Pearsall and Costigan, 1999; Riemer et al., 2008), meaning additional fictitious

forces are required to produce a simulated motion that replicates the experimental data. Several methods have been proposed to reduce

errors to improve dynamic consistency (Cahouët et al., 2002; Ganley and Powers, 2004; Kuo, 1998), including OpenSim's residual

reduction algorithm (RRA, https://simtk-confluence.stanford.edu/display/OpenSim/Residual+Reduction+Algorithm) that reduces the

fictitious, or "residual", forces and moments applied at the pelvis. RRA first computes changes to the total model mass as $\Delta m = F_{y,avg}/g$,

where $F_{y,avg}$ is the average vertical residual force across the simulation and g is acceleration due to gravity. RRA also calculates an

altered torso center of mass (COM) location to reduce residual moments in the frontal and transverse planes. In addition, RRA can

change the model joint accelerations slightly to achieve better dynamic consistency and further reduce residual forces and moments.

Thus, there is a tradeoff between the residuals and the kinematic errors, where the tradeoff is governed by user-selected tracking weights.

OpenSim's documentation recommends users manually adjust the tracking weights until the residuals are minimized, which is a time-

consuming process. In this paper we describe an open-source software tool (provided in Python and MATLAB) for optimization of

tracking weights in RRA, which provides biomechanics researchers with an automated method for selecting RRA tracking weights,

increasing efficiency in developing high-quality movement simulations.

2. METHODS

46   A Tracking Weight Selection Algorithm (TWSA) was developed to optimize the tracking weight values, which serve as inputs to

47   the optimization algorithm RRA in OpenSim. A modified random hill climbing algorithm was used to explore the search space.

2.1. OBJECTIVE FUNCTION FORMULATION

49   The TWSA minimized the sum of root-mean-squared (RMS) residual forces and moments and the sum of RMS kinematic tracking

50   errors as a weighted multi-objective cost function:

$$\min \quad W_R \sum_{i=1}^{m} (w_i R_i)^{p_R} + W_E \sum_{j=1}^{n} (w_j E_j)^{p_E} \qquad (1)$$

where R_i is the RMS of a residual term, W_R and W_E are the user-specified weights applied to the sums of the forces and errors, w_j and w_i

are the weights applied to individual errors and forces, E_j is the RMS of a particular error, p_R and p_E are user specified powers and m

and n are the number of residuals and errors examined respectively. Each RMS value is weighted by a user-specified value, w_i or w_j. By

default these weights are set to the inverse of 2cm for translational errors, 2° for rotational errors, 7.5% bodyweight (N) for residual

forces, and 1.5% bodyweight times one meter for residual moments in line with OpenSim recommendations (Hicks et al., 2015 and

OpenSim Documentation[1]). Thus, the weights serve to normalize the RMS errors to a desired threshold value. Errors above the threshold

result in a weighted value >1, while errors below the threshold result in weighted values < 1. The exponents p_R and p_E are applied to the

residuals and errors to cause errors above the threshold to rapidly increase the objective function value, while errors below the threshold

diminish in the objective function.

2.2. ALGORITHM DESCRIPTION

The TWSA minimized the residual forces and moments while tracking the experimental data. A set of uniform tracking weights

was used to perform the initial RRA and the objective function was evaluated in a MATLAB function and reported to the TWSA. This

first evaluation of the objective function was the current best solution. An array of parameters, $\vec{\tau}$, was then created to perturb tracking

weights. Each element in $\vec{\tau}$ was calculated as $\tau_i = b^t$, where b started at 1.5 and was lowered to 1.1 after 75% of the TWSA iterations

were performed, and t was an integer ranging from -2 to 2 selected from a random sample which was weighted to favor negative values

(decrease the tracking weight) if coordinate tracking was below a good threshold, positive values if tracking was bad (increase the

tracking weight), and equal chances otherwise. Each tracking weight was then multiplied by the corresponding τ_i to generate a new set

of tracking tasks, which were used to run the next RRA iteration. The objective function was evaluated after each iteration, and the

tracking weights corresponding to the current lowest objective function value were used as the starting weights that are perturbed for

subsequent iterations. This process was repeated until the cost function value was below a specified threshold or an iteration limit set by

---

[1] https://simtk-confluence.stanford.edu:8443/display/OpenSim/Getting+Started+with+RRA

the user was reached. The resulting solutions from the TWSA do not guarantee optimality but improve errors relative to baseline,

meaning that the solutions have lower residual forces and moments while still maintaining acceptable kinematic tracking errors (Hicks

et al., 2015).

2.3. TEST CASE

To test the effectiveness of the TWSA, we selected a single participant (subject01 - male, 72.84kg) from publicly available data

repository (simtk.org/home/nmbl_running, Hamner & Delp, 2013) for a common dynamic task: running. Three running strides each

were isolated from motion files of 2.0, 3.0, 4.0, and 5.0 m/s, and were used to develop the running simulations in OpenSim 3.3. The

TWSA was applied using two different models. First, the full body model with 29 degrees of freedom and 92 Hill-type musculotendon

actuators developed by Hamner et al. (Hamner et al., 2010; Hamner and Delp, 2013) was used because it was consistent with the

dataset. Next, the gait2392 model with 23 degrees of freedom and 92 Hill-type musculotendon actuators (Delp et al., 2007) was

selected because it is widely used and available with OpenSim installation. A key distinction between these models is that gait2392

uses a lumped head/arms/trunk segment, whereas the Hamner2010 model implements multi-segment arms. This difference in model

formulation can be used to demonstrate the robustness of the TWSA, as ignoring contributions of the arms during running introduces

additional dynamic inconsistency in the simulation. Following a typical workflow with ground reaction forces applied to the calcanei

and tracking a desired inverse kinematics solution, RRA was first run iteratively using fixed tracking weights, and recommended

model mass adjustments were performed to reduce average residual forces and moments applied to the pelvis until the total mass

change was less than 0.001 kg. Then, the TWSA was applied to each running trial using the mass adjusted model to further reduce the

magnitude of residuals. For this study, a fixed iteration number of 200 RRA iterations were performed by the TWSA, and the tracking

weights associated with the best objective function value were then re-run for the final RRA results. For all trials $W_E = 3$, $W_R = 1$, $p_R =$

3, and $p_E = 4$. Residuals after the TWSA were compared to residuals prior to the TWSA, but after the mass adjustments, to determine

simulation improvement. The peak net external force from each running trial was used to normalize residuals for evaluation (Hicks et

al., 2015), and both peak and RMS residuals were analyzed. Tracking errors were evaluated to ensure all coordinates were within

measurement error.

3. RESULTS

Mass changes were less than 0.5 kg for all trials using both the Hamner2010 model and the gait2392 model. Torso center of mass

changes were less than 6 cm for most trials, and adjustments were slightly larger for the Hamner2010 model (Table 1). Trial1 in the 2.0

m/s condition required the largest change in center of mass location (>10 cm for both models) during this portion of the conventional

RRA workflow.

Table 1. Changes made to the torso center of mass for each trial using both the Hamner2010 and gait2392 models. Values are reported
in cm as (x, z) pairs for the anterior (x) and medio-lateral (z) directions.
103

		Hamner2010			gait2392		
		Trial			Trial		
		1	*2*	*3*	*1*	*2*	*3*
Speed (m/s)	*2.0*	(15.7, -1.2)	(4.4, 1.3)	(5.9, 0.3)	(11.8, -0.7)	(2.8, 1.2)	(4.2, 0.4)
	3.0	(5.0, 1.3)	(3.6, 0.9)	(4.8, 1.0)	(3.5, 1.4)	(2.3, 1.0)	(3.1, 1.2)
	4.0	(3.5, 1.4)	(5.8, 1.6)	(4.6, 0.9)	(2.1, 1.5)	(4.0, 1.5)	(3.1, 1.0)
	5.0	(9.0, 2.2)	(4.9, 0.5)	(7.9, -0.4)	(6.3, 1.9)	(3.3, 1.1)	(5.6, -0.4)

After performing the standard RRA-based model adjustments, we ran the TWSA using MATLAB R2020a (The Mathworks, Inc.)

and OpenSim v3.3 (Delp et al., 2007, simtk.org) on a 3.60 GHz CPU with 12 logical processors to optimize tracking weights, with each

running speed condition (2.0, 3.0, 4.0, and 5.0 m/s) evaluated in parallel. The 200 iterations took the most time to complete during the

2 m/s condition, finishing in 2 hours and 4 minutes using the Hamner2010 model, and 49 minutes using the gait2392 model. TWSA

objective function values were substantially reduced in the first 50 RRA iterations and achieved reasonable convergence between 100

and 150 iterations (Fig. 1). However, gradual reductions continue to occur with more iterations, and the lowest objective function values

were produced in the last 50 iterations for all trials. Using both the Hamner2010 and gait2392 models, the TWSA produced objective

function values less than 2.5 on average for 3, 4 m/s trials. Average best objective function values were 8.99 and 5.84 at 2 and 5 m/s,

respectively, using the Hamner2010 model and were 5.28 and 8.26 using the gait2392 model at 2 and 5 m/s, respectively. Trial 1 at 2

m/s had the highest objective function value for both models, but the 2 m/s trials otherwise achieved values less than 1.1. In addition,

certain trials sporadically produced peaks in objective function values between 50 and 150 iterations of the TWSA, and these were most

pronounced using the Hamner2010 model (Fig. 1).

Figure 1. Objective function values for the tracking weight selection algorithm optimization at each RRA iteration using the Hamner2010 model (left) and gait2392 model (right). Three trials were averaged at each iteration for both models at all running speeds (blue dashed lines).

After tracking weight optimization, peak and RMS residuals were substantially reduced except for the FZ residual (Fig. 2). RMS forces were less than 1% peak external force and RMS moments were less than 0.35% peak external force times 1 meter for both models after tracking weight optimization when averaged across speeds, with improvement in all residuals except FZ (Table 2.). Residuals were slightly larger using the gait2392 model compared to the Hamner2010 model after tracking weight selection. In addition, the FY residual was improved more across all speeds when using the Hamner2010 model compared to gait2392 achieving both a lower peak (Fig 2.) and RMS value (Table 2).

129 Figure 2. Peak residual forces (top) and moments (bottom) averaged at each running speed and plotted before (pre) and after (post) the
130 tracking weight selection algorithm was applied. Error bars represent the standard deviation of three trials at each speed using the
131 Hamner2010 (left) and gait2392 (right) models.
132

133 Table 2. Root mean squared (RMS) residual forces and moments normalized to OpenSim recommended maximum values (Hicks et
134 al., 2015). RMS forces and moments are normalized to 5% and 1% respectively of the peak external force (net ground reaction force)
135 during each trial. Values reported are the average RMS of 3 trials for each running speed both before (Pre TWSA) and after (Post
136 TWSA) the tracking weight optimization using both models. Values above 1 indicate the residual exceeds recommended thresholds.
137

		Hamner2010						**gait2392**					
		FX	*FY*	*FZ*	*MX*	*MY*	*MZ*	*FX*	*FY*	*FZ*	*MX*	*MY*	*MZ*
	2.0 m/s	0.44	0.27	0.13	2.66	3.84	3.45	0.40	0.24	0.11	3.30	2.98	3.29
Pre	3.0 m/s	0.31	0.18	0.11	2.45	4.67	2.48	0.26	0.16	0.08	2.89	3.61	2.55
TWSA	4.0 m/s	0.41	0.20	0.14	3.03	4.78	2.42	0.35	0.19	0.08	3.19	2.91	2.30
	5.0 m/s	0.52	0.25	0.18	3.30	6.00	3.01	0.46	0.23	0.13	3.58	2.94	3.01
	2.0 m/s	0.24	0.11	0.11	0.80	0.11	0.17	0.22	0.18	0.09	0.64	0.87	0.06
Post	3.0 m/s	0.12	0.11	0.12	0.02	0.29	0.15	0.13	0.14	0.08	0.07	0.17	0.37
TWSA	4.0 m/s	0.04	0.07	0.15	0.21	0.24	0.16	0.15	0.16	0.08	0.27	0.26	0.24
	5.0 m/s	0.23	0.13	0.17	0.19	0.32	0.19	0.26	0.24	0.12	0.17	0.08	0.42

4. DISCUSSION

The TWSA performed well using two different musculoskeletal models and improved residual forces and moments by similar

amounts with each model. We performed 200 iterations of RRA within the TWSA, but this upper limit may not be necessary to obtain

comparable improvements in residuals. This upper limit can also be adjusted by the user. Other than for one trial in both 2 and 5 m/s

using the gait2392 model, the best objective function value was improved by less than 1 in the last 100 RRA iterations. While more

iterations will guarantee a broader search of the solution space, a "good enough" objective function value could be used as a threshold

to stop the TWSA regardless of the number of iterations performed. An objective value threshold implementation, also an option within

the tool, would allow researchers to use more computational time on trials with higher residuals, like the first 2 m/s trial in this study.

All residual moments were substantially improved by the TWSA, while improvements in residual forces differed between models

and directions. Some of this discrepancy between residuals may be attributed to the objective function formulation. The recommended

normalization for residuals is stricter for moments than for forces, and thus, the TWSA favors solutions with lower moment residuals.

In addition, the RMS residual forces were all below the recommended threshold used to weight the objective function contributions and

were not highly penalized. Force residuals in the Z direction were not substantially reduced for either model at any running speeds. Z

(medial/lateral) direction forces were lower than both X (anterior/posterior) and Y (vertical) forces prior to the TWSA, and thus

contributed less to objective function values compared to X and Y forces. Improvements in Y direction force residuals were greater

using the Hamner2010 model compared to gait2392. This difference suggests that the presence of arm swing dynamics in the

Hamner2010 model was leveraged by the TWSA to reduce residual vertical forces without introducing excessive kinematic tracking

errors. The residual forces and moments are trivial to reduce if the kinematics are not tracked, which results in very low residuals but

very high errors. The TWSA sought to balance reducing the residuals and reducing kinematic error. Trial1 at 2 m/s illustrates how this

balance of terms may limit the ability of the TWSA to achieve a low cost function value. Kinematic errors likely required greater

residuals reductions during this trial, and these errors are much larger than the weights used for normalization. The user must choose

whether to allow greater kinematic errors or accept the large residuals in this case and adjust weights accordingly, and output results

should be critically examined before implementing more in-depth simulation analyses.

Other algorithms have been used to automate RRA tracking weight selection using similar objective functions (e.g., Samaan et al.,

2016), and many different optimization approaches could be successfully applied to this application. While it is challenging to directly

compare the TWSA to others because different motions were used and cost function formulations are different, the kinematic accuracy

of our approach (see Appendix for full kinematic results) was comparable to other approaches (Samaan et al., 2016).

5. CONCLUSIONS

The TWSA provides a valuable new tool for efficiently computing optimal RRA tracking weights. This algorithm is an important

and practical contribution to the modeling and simulation community and may be used to improve the quality of musculoskeletal

simulations of human movement. The TWSA reduced residual forces and moments below established guidelines in a reasonably short

amount of time (<2hr), requiring little or no user input. Supporting documentation and code to implement the TWSA in both Python

and MATLAB are available for download at: https://github.com/FxnlBiomechLab/twsa-optimization-for-rra.

ACKNOWLEDGEMENTS

The authors would like to thank Daniel Anderson and Moriah Hunt for their contributions to the development of the initial TWSA

algorithm. The authors also acknowledge Amy Hegarty and Alexandra Newman for testing of the tool.

CONFLICT OF INTEREST

The authors have no conflicts of interest to declare.

REFERENCES
Cahouët, V., Luc, M., David, A., 2002. Static optimal estimation of joint accelerations for inverse dynamics problem solution. J.
Biomech. 35, 1507–13.

Delp, S.L., Anderson, F.C., Arnold, A.S., Loan, P., Habib, A., John, C.T., Guendelman, E., Thelen, D.G., 2007. OpenSim: Open-
source software to create and analyze dynamic simulations of movement. IEEE Trans. Biomed. Eng. 54, 1940–1950.
https://doi.org/10.1109/TBME.2007.901024

Ganley, K.J., Powers, C.M., 2004. Determination of lower extremity anthropometric parameters using dual energy X-ray
absorptiometry: the influence on net joint moments during gait. Clin. Biomech. 19, 50–56.
https://doi.org/10.1016/j.clinbiomech.2003.08.002

Hamner, S.R., Delp, S.L., 2013. Muscle contributions to fore-aft and vertical body mass center accelerations over a range of running
speeds. J. Biomech. 46, 780–787. https://doi.org/10.1016/j.jbiomech.2012.11.024

Hamner, S.R., Seth, A., Delp, S.L., 2010. Muscle contributions to propulsion and support during running. J. Biomech. 43, 2709–2716.
https://doi.org/10.1016/j.jbiomech.2010.06.025

Hicks, J.L., Uchida, T.K., Seth, A., Rajagopal, A., Delp, S.L., 2015. Is my model good enough? Best practices for verification and
validation of musculoskeletal models and simulations of movement. J. Biomech. Eng. 137, 020905-1-020905–24.
https://doi.org/10.1115/1.4029304

Kingma, I., Toussaint, H., 1996. Segment inertial parameter evaluation in two anthropmetric models by application of a dynamic
linked segment model. J. Biomech. 29, 693–704.

Kuo, A.D., 1998. A least-squares estimation approach to improving the precision of inverse dynamics computations. J. Biomech. Eng.
120, 148–59.

Pearsall, D.J., Costigan, P. a, 1999. The effect of segment parameter error on gait analysis results. Gait Posture 9, 173–83.

Riemer, R., Hsiao-Wecksler, E.T., Zhang, X., 2008. Uncertainties in inverse dynamics solutions: a comprehensive analysis and an
application to gait. Gait Posture 27, 578–88. https://doi.org/10.1016/j.gaitpost.2007.07.012

Samaan, M.A., Weinhandl, J.T., Bawab, S.Y., Ringleb, S.I., 2016. Determining residual reduction algorithm kinematic tracking
weights for a sidestep cut via numerical optimization. Comput. Methods Biomech. Biomed. Engin. 19, 1721–1729.
https://doi.org/10.1080/10255842.2016.1183123

Yamaguchi, G.T., 2005. Dynamic Modeling of Musculoskeletal Motion: A Vectorized Approach for Biomechanical Analysis in Three
Dimensions. Springer.

APPENDIX
208
209

Table A1. Largest root mean squared tracking error for each coordinate across all running speeds and trials using the Hamner2010 model.

Hamner2010					
Translational (cm)		pelvis_tx	pelvis_ty	pelvis_tz		
	Pelvis	0.92	1.14	0.97		
Rotational (deg)		pelvis_tilt	pelvis_list	pelvis_rotation		
	Pelvis	0.54	1.24	1.96		
		lumbar_extension	lumbar_bending	lumbar_rotation		
	Torso	1.61	2.28	2.16		
		hip_flexion	hip_adduction	hip_rotation	knee_angle	ankle_angle
	Right leg	1.99	1.19	0.19	0.85	0.19
		hip_flexion	hip_adduction	hip_rotation	knee_angle	ankle_angle
	Left leg	1.10	1.08	0.76	0.30	0.17
		arm_flex	arm_add	arm_rot	elbow_flex	pro_sup
	Right arm	0.38	0.80	0.13	0.53	0.15
		arm_flex	arm_add	arm_rot	elbow_flex	pro_sup
	Left arm	1.07	0.65	0.73	0.23	0.01

210
211

Table A2. Largest root mean squared tracking error for each coordinate across all running speeds and trials using the gait2392 model.

Gait2392					
Translational (cm)		pelvis_tx	pelvis_ty	pelvis_tz		
	Pelvis	1.12	0.69	1.05		
Rotational (deg)		pelvis_tilt	pelvis_list	pelvis_rotation		
	Pelvis	0.71	0.35	0.44		
		lumbar_extension	lumbar_bending	lumbar_rotation		
	Torso	1.66	1.00	0.85		
		hip_flexion	hip_adduction	hip_rotation	knee_angle	ankle_angle
	Right leg	0.48	0.45	0.29	0.61	0.06
		hip_flexion	hip_adduction	hip_rotation	knee_angle	ankle_angle
	Left leg	1.92	0.72	0.17	0.09	0.04

212
213

10