Multivesicular Release Increases the Efficiency of Information Transmission at Sensory Synapses

Ben James, Pawel Piekarz, José Moya-Diaz and Leon Lagnado*

Sussex Neuroscience, School of Life Sciences,

University of Sussex, Brighton BN1 9QG, UK

* Correspondence: l.lagnado@sussex.ac.uk

The statistics of vesicle release determine how information is transferred in neural circuits. The classical model is of Poisson synapses releasing vesicles independently but ribbon synapses transmit early sensory signals by multivesicular release (MVR) when two or more vesicles are coordinated as a single synaptic event. To investigate the impact of MVR on the spike code we used leaky integrate-and-fire models with inputs simulating the statistics of vesicle release measured experimentally from retinal bipolar cells. Comparing these with models of independent release we find that MVR increases spike generation and the efficiency of information transfer (bits per spike) over a range of conditions that mimic retinal ganglion cells of different time-constant receiving different number of synaptic inputs of different strengths. When a single input drives a neuron with short time-constant, as occurs when hair cells transmit auditory signals, MVR increases information transfer whenever spike generation requires depolarization greater than that caused by a single vesicle. This study demonstrates how presynaptic integration of vesicles by MVR can compensate for less effective summation post-synaptically to increase the efficiency with which sensory information is transmitted at the synapse.

Introduction

The fundamental units by which information is encoded and transmitted in the nervous system are spikes and synaptic vesicles. Electrophysiology has allowed the spike code to be studied in detail (Gerstner et al., 1997; Quian Quiroga and Panzeri, 2009; Schwartz et al., 2006), especially in the context of the representation of sensory information (Carleton et al., 2010; Gollisch and Meister, 2008; Kayser et al., 2009), but less is understood about the vesicle code operating at excitatory synapses that drive spiking (Manwani and Koch, 2001; Rusakov et al., 2020; Zador, 1998).

Theoretical and computational approaches to understanding how synapses transfer sensory information have been based largely on the idea that changes in presynaptic potential are communicated by modulating the mean rate of a Poisson process in which vesicles at the active zone are triggered to fuse independently (Johnson, 1996; Pillow et al., 2005; Schwartz et al., 2006). When the release probability is low, this scenario can be simplified further to the idea of "one-spike-one-vesicle" to create a purely binary output in which a spike invading the active zone sometimes triggers release of a single vesicle and sometimes none (Lisman et al., 2007). More recently, however, a range of experimental evidence has demonstrated that synapses at many sites in the brain do not follow these simple behaviours but can also release two or more vesicles within milliseconds - a process termed multivesicular release (MVR). MVR has been observed in the hippocampus (Christie and Jahr, 2006), cerebellum (Auger et al., 1998) and somatosensory cortex (Holler et al., 2021; Huang et al., 2010) and is also a fundamental feature of ribbon-type synapses specialized to transmit signals in the first stages of vision and hearing, where it does not obey Poisson statistics (Glowatzki and Fuchs, 2002; Hays et al., 2021; James et al., 2019; Lagnado and Schmitz, 2015; Neves and Lagnado, 1999; Singer et al., 2004). A recent combination of electrophysiology with correlative light-and electron-microscopy has even led to the suggestion that MVR may contribute to synaptic transmission throughout the nervous system (Holler et al., 2021).

The closer together in time vesicles are released at a single synaptic connection the more effectively they will summate on a postsynaptic dendrite to impact the spiking activity of the target neuron. This simple idea has profound implications for understanding how information is transmitted in the brain because in principle it might allow for a sensory stimulus to be represented not just by the frequency of synaptic events (a temporal code) but also by their *amplitude* (Holler et al., 2021; James et al., 2019; Lisman et al., 2007). Direct evidence for amplitude coding at a synapse has been provided by improvements in the optical imaging of glutamate in the retina, which provide the resolution to count vesicles as they are released from individual active zones. This approach reveals that visual information can be represented both in the rate of vesicle release and in the number of vesicles released within each event, with larger and rarer events carrying the most information per vesicle (James et al., 2019).

How does MVR impacts on spike generation in the target neuron? An experimental investigation of this question is difficult because it would require spikes to be recorded post-synaptically while also characterizing the influence of individual active zones monitored with a resolution of single vesicles. We have therefore started with a modelling approach in which a train of synaptic events is simulated based on experimentally measured statistics of vesicle release and used as the input to a Leaky Integrate-and-Fire (LIF) model of the post-synaptic neuron (Abbott, 1999; Burkitt, 2006a, b; Gerstner et al., 1997). We gather these statistics from the ribbon-type synapse of retinal bipolar cells across which visual information is transmitted to post-synaptic ganglion cells, but the results can also be generalized to the transmission of auditory information from the ribbon synapses of hair cells.

We find that over a range of conditions MVR increased the number of spikes per vesicle compared to a simple rate-code in which all vesicles were released independently. The relative efficiency of information transfer, quantified as bits carried by the spiking response per vesicle released, differed between the two synaptic coding strategies by amounts that depended on the time-constant of the target neuron and the reliability of the

synaptic inputs. MVR tended to be advantageous when i) the neurons time-constant was shorter, causing less post-synaptic summation of synaptic potentials at physiological rates of vesicle release, and ii) individual synaptic inputs were more reliable so that a lower degree of convergence was required to depolarize the target to threshold for a given stimulus strength. The general picture is that presynaptic integration of vesicles by MVR can compensate for less effective summation post-synaptically to increase the efficiency with which sensory information is transmitted at the synapse.

Methods

Modelling Overview

Modelling the effects of MVR on spiking involved the following basic steps:

1. Statistics of vesicle release in retinal bipolar cells responding to visual stimuli. Using iGluSnFR expressed in retinal bipolar cells of larval zebrafish, we measured the amplitude of synaptic events and their timing relative to a sinusoidal full-field stimulus of varying contrast (Fig. 1A).   At each contrast we calculated i) the average rate of vesicle release over a 30 s period R (Fig. 1B); ii) the probability of events composed of different numbers of quanta, P_{Qe} (Fig. 1C), and iii) the "temporal jitter" of events of each amplitude, quantified as the standard deviation of event times relative to any particular phase of the sinusoidal stimulus ($TJ(Q)$, Fig. 1D-F).

2. Simulation of synapse output using Gaussian statistics. Based on step 1, two types of simulated synaptic output were constructed: one in which stimulus contrast was represented as a "pure" rate-code in which all vesicles were released independently and a second "hybrid code" in which amplitude also varied (Fig. 2A). In both cases, the overall average rate of vesicle release R was fixed to values measured experimentally at a given contrast.

Figure 1. Multivesicular Release in the Retina of Zebrafish. A. Left: Multiphoton image of BCs in the retina of a larval zebrafish. They are visualized by the iGluSnFR reporter in the surface membrane. Middle: Two BCs at higher magnification. The mosaic expression of the reporter allows for distinguishing individual BCs and distinguishing glutamate release at different synapses. Right Top: Recorded fluorescence time series from an individual active zone. Bottom: Estimated quantal content of the time series above. Note the heterogeneity in the response amplitude, corresponding to variable quanta released per event. **B.** Normalized change in the rate of events (black) and average event amplitude in quanta (red) (60 synapses). **C.** Distribution of event amplitudes during a 30 s application of a 5 Hz stimulus at 80% contrast (60 synapses), truncated to only include events containing fewer than 11 quanta. **D.** Quantal time series (black lines) in response to a 5 Hz, 80% contrast full-field stimulus (red), with blue dashed lines present only for ease of visibility. Note that events composed of four or more vesicles occur in a temporally small window during each cycle, while lower quantal events are more temporally dispersed. **E.** The temporal jitter as a function of quanta in event for a 100% contrast stimulus**. F.** Mean-shifted distribution of events containing 5 or more quanta (black) and of events containing one quantum (red) in response to a 30 s, 5 Hz, 100% contrast sinusoidal stimuli. Results compiled from a total of 60 synapses after mean shifting.

Figure 2. Overview of modelling. A. A leaky-integrate-and-fire neuron received either rate (top) or hybrid (bottom) inputs. **B.** Illustration of release simulation for the Gaussian Model. The number of vesicles in an event (for the MVR case) or the number of released uniquantal events (for the rate case) is sampled from the distribution P_Q. For the MVR case, each event is then given a time by sampling from a Gaussian Distribution with variances set by the mean temporal precision of events, given by TJ(q). For the rate case, a corresponding number of event times are sampled from the distribution of uniquantal event times (bottom middle). **C.** The sampled event time and amplitude tuples are then convolved with a synaptic current filter. The resulting current is summed over the number of inputs to the cell. Plotted on the right are the average synaptic current input to a cell utilizing a rate code (red) and hybrid code (black). Note the increased temporal variability in the rate code (SD = 360 ms for the hybrid case vs. 685 for the hybrid case). **D**. Demonstration of the Poisson release model. Bottom: intensity function driving the rate of vesicular events. Middle: expected number of vesicles released in an event as a function of time. Top: Expected cumulative vesicles released as a function of time for rate and amplitude codes, offset for visualization. These functions have been equalized by design. **E.** Expected total vesicles released over a one second window as a function of stimulus 'contrast'.

The output of a synapse employing MVR was generated by randomly selecting a total of N events with amplitudes chosen from the distribution of quanta in an event P(Qe) (Fig. 2B). The time of each event relative to the stimulus was then set with a temporal precision

dependent on its amplitude, defined by TJ(Qe). The output was constrained to be

composed of only one or zero events per cycle of the stimulus, with the probability of no

event given by $p_Q(f, c)$. The output of a hybrid synapse employing MVR was therefore

described as a vector E of event times and a vector Qe of event amplitudes, both of length

N. The rate-code comparison was constructed by replacing each event consisting of

more than one quantum with an equivalent number of uni-quantal events, each event time

now sampled from the distribution of times of uniquantal events (Fig. 2B). The vectors

describing a pure rate synapse were therefore of variable lengths corresponding to the

total number of vesicles sampled within the 30 s sample period. The resulting vectors Qe

and E of event quanta and event times were then passed into a conductance-based

model LIF model (Fig. 1) and the spike output analysed.

3.   *Simulation of synapse output using marked Poisson Processes.* For purely rate-

coded synapses, we used a Nonhomogeneous Poisson Process (NHPP) as the driving

force for vesicle release, in which the mean rate λ(t) varied sinusoidally in time. By

definition, simple Poisson Processes describe a situation in which all events occur

independently and with exponentially distributed interevent times and cannot, therefore,

be used to model MVR when two or more vesicles are released within a single synaptic

event. To construct an amplitude-modulated Poisson Process we turned to a modification

known as Poisson Splitting or Location-dependent thinning (Resnick, 1992), where events

can be assigned a type based upon their location in time (Supplementary Figure 1). In this

case events occur with a constant rate but the number of vesicles in each event is chosen

based upon when the event occurred. We could therefore drive the LIF model neuron in

two distinct regimes: a pure rate case, where all information is encoded by modulating the

mean rate of release of individual vesicles and a hybrid case, where information is

encoded by modulating both the rate and quantal content of synaptic events.

A key aspect of our investigation was to construct the rate and hybrid models in such

a way that each released the same average number of vesicles, with differences found

only in the variabilities. In other words, vesicles were released individually in the "rate

code", but in packets of variable size in the "hybrid code". To simulate pure rate-coded

synaptic inputs case, we used a sinusoidal intensity function. The response of each

synapse to varying contrasts was simulated by increasing the amplitude of the sinusoid

between a total release of between 5 vesicles s^{-1} at input condition 1 (which we term 10%

contrast below) and 65 vesicles s^{-1} at input condition 10 (100% contrast; Fig. 2D and E).

for the rate case. Responses from multiple cells were assumed to come from the same

distribution, and as such we simulated the responses of multiple BCs onto a single cell by

summing the individual responses. To simulate hybrid coding we used a binomial

compounding function with a constant N=10, where the probability of release is a sinusoid

resulting in equivalent average release rates.

4.   A conductance-based Leaky Integrate-and-Fire (LIF) model of the post-synaptic

neuron. The vectors describing amplitudes and times of synaptic events were convolved

with a synaptic filter to estimate the time-course of the synaptic current S$_{in}$ (Fig. 2C) which

was then passed through a Leaky Integrate-and-Fire model to calculate the change in

voltage and spike output. LIF models provide a computationally compact method for

exploring basic physiological parameters affecting spiking, including the number of

synaptic inputs, cell time-constant, threshold relative to resting potential and ion channel

conductances (Abbott, 1999; Burkitt, 2006a, b; Gerstner et al., 1997). Voltage is

governed by the differential equation:

$$I(t) = g_l\big(v_{rest} - v(t)\big) + \big(v_e - v(t)\big)g_e S_{in}(t) \qquad \textbf{(1)}$$

Where g_l is leak conductance, g_e is excitatory conductance, v_e is the excitatory reversal

potential, and v_{rest} is the resting membrane potential. The synaptic input, S_{in}, is defined

by the convolution of an alpha current impulse function with the input s(t),

$$S_i n(t) = \alpha * s(t) = \sum_{i=1}^{n} \alpha(t - t_i) \qquad \textbf{(2)}$$

Where s(t) is the sequence of Dirac delta function describing the timing of each event in a

realization of the Process, and

203
$$\alpha(t) = \left(\frac{t}{\tau_s}\right) - exp\left(\frac{-t}{\tau_s}\right)$$
(3)

describes the time course of synaptic current. Here, we used a value of τ_s = 2 ms

(Destexhe and Rudolph, 2004) which yields a total conductance of 2 nS per quanta. Once

the cell hits a threshold θ, it fires a spike and the voltage is immediately reset to the reset

potential v_{reset} , and remains at that value in a refractory period for τ_{ref} = 5 ms. There is

no explicit membrane time-constant ($\tau_m = RC$) in a conductance model but the time

course of the leak can be described as the reciprocal of the leak conductance $\tau_l = g_l^{-1}$.

Due to its similarity with the current-based model, we will describe the model in terms of

τ_l.

Parameter (symbol)	Simulated Value/s
Vesicles Required to Spike, k	10, 25, 50,100 vesicles
Leak Constant, τ_l	1, 10, 20, 50 ms
Resting Potential, v_{rest}	-70, -65, -50, -55 mV
Excitatory Reversal Potential, v_e	0 mV
Spiking Threshold, θ	-50, -45, -40, -35 mV
Number of Inputs, N	50, 100, 250, 500
Refractory period, τ_{ref}	5 ms
Synaptic Time Constant, τ_s	2 ms
Stimulus Frequency, f	5, 10, 15 Hz
Stimulus Contrast, c	20, 60, 100%

Table 1: Simulation Parameters. Parameters used for simulations, with ranges based upon experimentally

recorded values (Destexhe and Rudolph, 2004; O'Brien et al., 2002; Pillow et al., 2005)

To compare how the MVR might shape the spike output of a postsynaptic cell across

a range of physiological values, we systematically varied the parameters shown in Table

1. Note that here, rather than representing the set of the excitatory conductances, g_e, we

computed the approximate leak conductance required for the cell to spike in response to k

vesicles in a perfect integrator – with corresponding g_e values ranging in the 1-100 nS

range. In the retina, bipolar cells transmit to RGCs of widely varying size and electrical

properties. In mice, for instance, input resistances of RGCs can vary from dozens of MΩ

to a GΩ, with values of the membrane time-constant ranging from less than 5 ms to over

50 ms (O'Brien et al., 2002). At another extreme, primary auditory afferents receive inputs

from single active zones delivering the output from hair cells and have input resistances of

GΩ leading to the suggestion that a single glutamatergic vesicle is sufficient to trigger a

spike (Fuchs and Glowatzki, 2015; Glowatzki and Fuchs, 2002). Thus, the number of

vesicles sufficient to generate a spike in a cell postsynaptic to a ribbon synapses (k)

varies from one to hundreds.

5. ***Analyzing the spike output of the model neuron.*** We concentrated on three

aspects of the spiking response of the model neuron: the spike count generated by each

cycle of the 5 Hz stimulus, the temporal accuracy of spikes and the average rate of

information transfer about the modulation in stimulus strength (i.e contrast).

Temporal accuracy was quantified as "temporal jitter" (TJ, in ms), which was in turn

calculated from the Vector Strength (VS), which takes values between zero and one, with

zero being complete independence from the stimulus and one being perfect phase-locking

(Baden et al., 2011; Goldberg and Brown, 1969). VS was computed for each quantal

event type in response to a 30 s stimulus of varying contrast delivered at 5 Hz, with the

equation:

$$VS_Q = \frac{1}{N_Q}\sqrt{\left(\sum_{i=1}^{N_Q} cos\left(\frac{2\pi t_{Q_i}}{T}\right)\right)^2 + \left(\sum_{i=1}^{N_Q} sin\left(\frac{2\pi t_{Q_i}}{T}\right)\right)^2}$$ **(4)**

where t_{Q_i} is the phase of the ith event of quantal content Q, and T is the stimulus period.

VS can then be easily converted to Temporal Jitter (TJ) by:

246
$$TJ_Q = \frac{\sqrt{2(1-VS_Q)}}{2\pi f} \tag{5}$$

247   We calculated the mutual information (Shannon, 1948) between the stimulus S and

248   either the spike times or the total number of spikes occurring over a period of 200 ms (N,

249   corresponding to one cycle of the 5 Hz stimulus, 2 cycles of the 10 Hz stimulus or 3 cycles

250   of the 15 Hz stimulus).   Mutual information for spike counts was computed empirically

251   from the joint and marginal distributions $p(s, n)$, $p(n)$, and $p(s)$ as:

252
$$I(S; N) = \sum_{s \in S, n \in N} p(s, n) log\left(\frac{p(s,n)}{p(s)p(n)}\right) \tag{6}$$

using the direct approach (Victor, 2006). Each stimulus s is has one of three contrasts and

one of three frequencies, leading to a total of 9 different stimuli and a maximum of ≈ 3.17

bits of information.   The total mutual information was calculated by discretising the

response in a 200 ms time window into 5 ms bins, yielding a total of 40 response bins and

2^{40} possible responses (the vast majority of which are never observed). To reduce bias in

the estimates, each simulation was run a total of 1000 times, with typical simulations

generating under 80 unique responses. Keeping the ratio of the number of samples to the

number of distinct responses large ensures any bias is small (Panzeri et al., 2007). The

spike count information was computed similarly, using the distribution of spike counts **N**.

Finally, the spike-time information was computed as the difference between the total

information and the spike count information, $I(S; R)_{Time} = I(S; R)_{Total} - I(S; R)_{Count}$

The signal-to-noise ratio associated with a change in the rate of a Poisson process

Imagine the mean rate of a Poisson process, R, changes by a factor a. The signal, S,

generated by comparing two observation times Δt will be the change in the mean number

of events counted in each period (aR Δt - R Δt), and the variance in that signal will be the

sum of the number of events counted in each period (aR Δt + R Δt). Defining the SNR in

the same way as the discriminability (d') used in signal detection theory, we have

$$SNR = \frac{S}{\sqrt{variance}} \qquad (\textbf{7})$$

273   yields

$$SNR = \frac{(aR\Delta t - R\Delta t)}{\sqrt{(aR\Delta t + R\Delta t)}} \qquad (\textbf{8})$$

275   which can be rearranged to obtain the time period Δt required to obtain a given SNR, as

$$\Delta t = \frac{SNR^2}{R} \frac{(a+1)}{(a-1)^2} \qquad (\textbf{9})$$

Multiphoton imaging of glutamate release

Methods for *in vivo* imaging of glutamate release in the retina of zebrafish were as

described previously (James et al., 2019). Transgenic larval zebrafish expressing the

iGluSnFR reporter under the *ribeye a* promoter were imaged at 7-9 days post-fertilization

after embedding in a 3% low melting-point agarose in E2 on a glass cover-slip. To

prevent eye movements, the fish was injected with 1 nL of alpha-bungarotoxin behind the

eye. Imaging was carried out using a multiphoton microscope (Scientifica) equipped with

a mode-locked titanium–sapphire laser (Chameleon, Coherent) tuned to 915 nm and an

Olympus XLUMPlanFl ×20 water immersion objective (NA of 0.95). Fluorescence

emission was also collected using a sub-stage oil condenser (Olympus; NA of 1.4), which

was essential to achieve a SNR adequate for reliable detection of single vesicles.

Light emission was filtered through GFP filters (HQe525/50, Chroma Technology)

before detection using GaAsP photomultipliers (H7422P-40, Hamamatsu). Photocurrents

were passed to a current-to-voltage converter, after which signals from the objective and

condenser were summed and digitized through ScanImage (v.3.6; Vidrio Technologies).

For this work, all time-series were acquired as 128 pixel line scans imaged at 1 kHz and

analysed in custom software written within IgorPro (Wavemetrics). Stimuli were generated

by an amber LED (peak wavelength of 590 nm) filtered through 590/10 bandpass filter (Thorlabs) delivered through a light-guide placed near the fish's eye, with the mean stimulus intensity of ~320 nW mm^{-2}. Detailed evidence that this approach can detect the release of single vesicles from individual active zones has been presented previously (James et al., 2019).

Results

Synaptic coding of a sensory stimulus: gathering release statistics for an empirically-driven model

Our aim was to investigate how the statistical properties of vesicle release affected the synaptic transfer of sensory information, comparing synapses employing MVR with the conventional view of synapses operating as Poisson machines. The starting point was to gather experimental measurements of release statistics from retinal bipolar cells expressing the glutamate reporter iGluSnFR, and examples of such records are shown in Fig. 1A. Both the rate and amplitude of glutamate transients varied widely during sinusoidal modulations in light intensity.

We measured how changes in contrast altered three aspects of the vesicle code highlighted in Fig 1: event rate R(Q), distribution of event amplitudes P(Qe), and variability of event timing TJ(Q). R saturated at a lower contrasts than Qe, such that contrasts greater than ~50% were often encoded entirely by the number of vesicles released within an event (Fig. 1B and C). A potential role of MVR in determining the temporal accuracy of spiking in the post-synaptic neuron is immediately suggested by the observation that multiquantal events were more tightly phase-locked to the stimulus than vesicles released individually (Fig. 1D-F). Uniquantal events had a temporal jitter of 21.2 ± 1.5 ms, while events composed of 9 quanta had a temporal jitter of just 2.7 ± 0.6 ms, which is very similar to the precision of spikes observed in RGCs of the salamander retina responding

to a high-contrast stimulus (Berry et al., 1997a; Uzzell and Chichilnisky, 2004). The

relation between TJ and Qe is shown in Fig. 1E and a comparison of the distribution of

times for uniquantal and multiquantal events is shown in Fig. 1F.

Based on these measurements we constructed two types of synaptic input to the

model neuron: purely rate-code inputs in which all vesicles were released independently

(red in Fig. 2A) and hybrid inputs in which both rate and amplitude of events varied (black;

see Methods). To compare how these two coding strategies performed with equivalent

resources the average rates of vesicle release were fixed for both types of input at the

values measured experimentally at a given contrast and frequency (Fig. 1B). Measuring

the output of individual synapses to stimuli of different contrasts allowed us to then make

measures of the mutual information between the stimulus set and spikes generated in

model neurons.

The effects of multivesicular release in a "small" cell and "large" cell

Bipolar cells transmit the visual signal to RGCs that vary in widely in the area of their

dendritic trees and, therefore, their receptive fields. In the fovea of primates, for instance,

midget ganglion cells are electrically compact and receive 25-50 synaptic inputs from

between one and three bipolar cells (Calkins et al., 1994; Kolb and Marshak, 2003). But

in the periphery of the retina, RGCs have larger dendritic fields and receive inputs from

hundreds of bipolar cells, with up to thousands of synapses (Jacoby et al., 2000). To

illustrate how MVR might impact on the spike output of these different post-synaptic

neurons we begin by comparing responses in a synthetic 'midget' RGC ($\tau_l = $ 5 ms with 50

synaptic inputs; Fig. 3A-E) and a larger 'peripheral' RGC ($\tau_l = $ 50 ms with 500 inputs; Fig.

3F-J) responding to a 5 Hz stimulus.

Figure 3. Effects of multivesicular release on spike generation in a "midget" cell and a "peripheral"
cell.

A. Raster plots (top), example voltage traces (middle), and example synaptic input (bottom), for
hybrid and rate code driven cell at 100% contrast at 5 Hz. One cycle of the sinusoidal stimulus is
shown. This was a "small" cell simulated with: inputs = 50, k = 10, τ_l = 5 ms, v_e = 0, θ = -50 mV,
v_{rest} = -70 mV. The number of vesicles required to generate a spike (k) was 10. **B.** Same as **A**, but
for 20% contrast. **C.** Mean spike count as a function of stimulus contrast (± standard deviation).
Note the strongly supralinear relation. Synapses employing MVR begin to trigger reliable spiking at
40% contrast, while purely rate-coded synapses begin at >60%. **D.** Spike time distribution for rate
(red) and hybrid (black) codes in response to a 5 Hz stimulus at 100% contrast as in **A**. **E.**
Distribution of interspike intervals for 100% contrast, which were significantly shorter in the hybrid
case (9.7 ± 2.5 ms) than the rate case (11.75 ± 2.62 ms, Paired Wilcoxon Rank Sum, p < 0.05). **F-**
J. Corresponding to A-E, but for a "large" cell simulated with: inputs = 500, k = 100, τ_l = 50 ms, v_e
= 0, θ = -50 mV, v_{rest} = -70 mV, k = 100. The majority of rate code trials generate five spikes, while
the majority of hybrid code trials generate only four spikes (F). The spike count in the cell driven by
rate-coded synapses was proportional to stimulus contrast (slope of 0.03 spikes/percent contrast).
Note the increased temporal precision of the rate code, with the first peak variance of 1.56 ± 0.23
ms compared to 6.95 ± 0.83 ms for the hybrid code.

In the midget cell, MVR increased the efficiency with which vesicles drove spikes as

well as the maximum frequency of spiking. Across all contrasts but the lowest, the cell

receiving inputs from hybrid synapses generated more spikes than the equivalent cell

receiving purely rate-coded inputs ($p < 0.013$, Wilcoxon Signed-Rank test; Fig. 3A-C). The

rate code failed to generate spikes reliably at all but the highest contrasts, while the hybrid

code drove responses starting at 40% contrast (Fig. 3C). The mean first spike latency

was not affected by coding strategy (Fig. 3D), but the distribution of interspike intervals at

100% contrast was significantly shorter in the hybrid case (9.7 ± 2.5 ms) than the rate

case (11.8 ± 2.6 ms, $p < 0.05$, Wilcoxon Signed-Rank. test; Fig. 3E).

Simulations of the peripheral RGC (Fig. 3F-J) demonstrated two key functional

differences compared with the small, both of which recapitulated experimental

observations in the retina of primates: spike rates were higher at any given contrast (Fig.

3H; Kaplan and Shapley, 1986) and the time to peak response was shorter (Fig. 3I; Sinha

et al., 2017). In this case, the synaptic coding strategy had little effect on the total number

of spikes generated by a stimulus (Fig. 3H) but it did affect temporal precision: the first

peak in the distribution of spike times had a standard deviation of 1.56 ± 0.23 ms with

rate-coded inputs compared to 6.95 ± 0.83 ms for synapses employing MVR (Fig. 3I).

Recapitulating observations in the midget cell, interspike intervals were shorter when the

larger neuron was driven by hybrid synapses (Fig. 3J).

These examples show how the impact of MVR on the spike code of the post-synaptic

neuron depends on its membrane time-constant: in a midget RGC with shorter τ_l MVR

tended to increase spike count but in a peripheral RGC with longer τ_l it tended to improve

the temporal precision of spikes. The maximum spike rate, however, was always higher

in the neuron driven by synapses exhibiting MVR.

MVR increases spike count over a range of conditions

RGCs with larger receptive fields and dendritic trees receive larger numbers of synaptic

inputs (N) and changes in the degree of convergence will be a key factor in determining

the efficiency of spike generation. A second key variable is the average strength of

synaptic responses, which in turn depends on the strength of the stimulus.   In our

modelling framework synaptic strength is directly related to k, the minimum number of

vesicles that would need to be summed instantaneously to depolarise the neuron to

threshold. Although we systematically varied both k and N (Table 1) we found the ratio

k/N to be a useful summary metric that reduced dimensionality of the data while providing

insight into the effects of both synapse strength and the degree of convergence. For

instance, depolarization of the target neuron to threshold might occur by integrating

signals from just a few synapses with a high probability of response (i.e reliable synapses)

or more synapses with lower average response (i.e synapses of lower reliability).

Medium-sized RGCs in guinea-pigs receive about 1000-2000 inputs, and a brief burst of

excitation comprising 3-65 vesicles triggers a burst of 1-6 spikes (Freed, 2005).   This

example therefore provides an upper limit of k ~10 and k/N is ~0.01. In contrast, a midget

RGC might receive just 10 inputs. If the same number of vesicles are required to trigger a

spike, k/N = 1, and even if just one vesicle is sufficient, k/N =0.1.

Increasing τ_l always increased the spike count over the 200 ms time window, and this

is shown in Fig. 4A (top) for an example neuron with 500 inputs requiring the summation

of 100 vescles to trigger a spike (k/N = 0.2).   The absolute difference in spike count

between hybrid inputs and rate-coded inputs are shown below, demonstrating that for this

value of k/N, the hybrid code produces more spikes than the rate code when τ_l is less

than ~15 ms. The pattern of interaction between τ_l and k/N is shown for hybrid coded

inputs in Fig. 4B and the rate-coded inputs in Fig. 4C: in both cases, the lower the

average number of vesicles released per synapse to trigger a spike the larger the total

spike count for a cell of given time-constant.   But the size of these changes were not the

same and the difference between the counts generated by hybrid- and rate-coded inputs

is shown in Fig. 4D. For a given τ_l, rate-coded inputs generate more spikes at lower k/N

and hybrid inputs were more efficient at higher k/N (i.e when spikes were generated by

activation of a larger proportion of inputs).

This comparison revealed a clear pattern: the rate code outperformed the hybrid code

only when synapses were relatively unreliable. As the average number of vesicles

released per synapse increased, a regime was entered in which the hybrid code

generated spikes with greater efficiency (i.e more spikes per released vesicle), after which

the coding strategy did not affect the spike count. In other words, where spike generation

required more reliable synapses, reflecting a higher k/N ratio, it often became more

effective if summation began *presynaptically* by the process of MVR.

Figure 4. Hybrid coding increased spike count over a range of physiologically-relevant conditions

A. Top: Mean spike count as a function of leak time-constant $(\tau)_l$ for a cell receiving N=500 inputs and

requiring k=100 vesicles to spike in response to a 5 Hz stimulus of varying contrast (other parameters as in

the "large peripheral" cell in Fig. 3). This count is over a 200 ms time window so can be multiplied by 5 to

obtain spike rates. Bottom: Spike Count Difference (Hybrid – Rate) from the data in top panel. For this ratio

of k:N, the hybrid code produces more spikes than the rate code when $\tau_l < 15$ ms. **B.** Top: heat map showing

the spike count generated by hybrid inputs for cells of varying k/N and τ_l for a stimulus of 20% contrast.

Counts were averaged over values of k and N shown in Table 1. Bottom: as top but for 80% contrast. **C.** As B

but for rate-coded inputs. Note again that the average rate of vesicle release was the same as in B for a given

contrast. **D.** The difference between the counts generated by hybrid- and rate-coded inputs in B and C. Note

that, for a given τ_l, rate-coded inputs generate more spikes at lower k/N and hybrid inputs were more efficient

at higher k/N.

How does this comparison of the hybrid and rate codes relate to the physiology of

synapses transmitting the visual signal? Compared to other visual circuits, such as those

in the cortex, the retinal output is strikingly reproducible over repeated trials of a stimulus

and contrasts of 20-40% can trigger spikes in RGCs of a variety of species with almost

perfect reliability (i.e close to 100% of trials; Berry et al., 1997a; Gollisch and Meister,

2008)).   Unsurprisingly, the reliablity of individual bipolar cell synapses was lower. At 20%

contrast a 5 Hz stimulus triggered a response in 31 ± 3% of stimulus cycles (N = 48

synapses), rising to 64 ± 4% of cycles at 60% contrast (N = 56 synapses). Experimental

measurements of the average number of vesicles released per stimulus at these contrasts

(where N is a single synapse) are shown in Fig. 1A-B: a stimulus of 20% contrast released

an average of 2.32 ± 0.09 (N = 48 synapses) vesicles per synapse, while 60% contrast

released 2.84 ± 0.14.   Synapses transmitting the visual signal to the inner retina are

therefore operating over a range reliabilities where MVR provides a distinctive advantage

over a pure rate-code by increasing the number of spikes generated per released vesicle.

The consequences on the information carried by the spike response will be discussed

below (Fig. 7).

The flip side of the results in Fig. 4D is that a pure rate-code will be more effective

than MVR in situations where the neuron is driven by synapses where k/N less than ~0.15

i.e where convergence of a larger number of less reliable synapses is required for

depolarization to threshold. In mammals, this is the situation when the visual signal

reaches the primary visual cortex: excitatory synapses onto pyramidal cells have an

average release probability of ~0.17 vesicles per presynaptic spike (Allen and Stevens,

1994; Smetters and Zador, 1996) and these synapses operate with a high coefficient of

variation.   The unreliability of cortical synapses is therefore a major source of noise that

impacts on information transfer (Branco and Staras, 2009; Moreno-Bote, 2014; Rusakov

et al., 2020; Allen and Stevens, 1994; Smetters and Zador, 1996).

MVR reduces spike latency over a range of conditions

Visual information is contained not only in the number of spikes generated by a stimulus

but also in their timing (Butts et al., 2011; Gollisch and Meister, 2010), which can be

precise to within a few milliseconds in RGCs (Berry et al., 1997a; Uzzell and Chichilnisky,

2004), the LGN (Reinagel and Reid, 2002) and visual cortex (Buracas et al., 1998). In

RGCs, the temporal precision of spiking allows the latency to the first spike to transmit

more information about a stimulus than the total number of spikes, at least when a

stimulus drives episodic responses (Gollisch and Meister, 2008). To assess the impact of

MVR on the temporal precision of spike generation we therefore analyzed how τ_l and k/N

affecting first spike latencies (Fig. 5).

Figure 5. Hybrid coding reduced spike latency over a range of physiologically-relevant conditions

A. Top: Mean first spike latency as a function of leak time-constant $(\tau)_l$ for a cell receiving N=500 inputs and

requiring k=100 vesicles to spike in response to a 5 Hz stimulus of varying contrast (other parameters as in

the "large peripheral" cell in Fig. 3). Latencies were measured relative to an arbitrarily chosen phase of the

sinusoidal stimulus so it is the change in these values that is most informative. Bottom: Latency Difference

(Hybrid – Rate) from the data in top panel. For this ratio of k:N, the hybrid code produced at greater latency

when τ_l > 15 ms. **B.** Top: heat map showing the average first spike latency generated by hybrid inputs for

cells of varying k/N and τ_l for a stimulus of 20% contrast. Latencies were averaged over values of k and N

shown in Table 1. Bottom: as top but for 80% contrast. **C.** As B but for rate-coded inputs. **D.** The difference in

first spike latency generated by hybrid- and rate-coded inputs in B and C. For a given τ_l, rate-coded inputs

generated faster responses at lower k/N while hybrid inputs generated faster responses at higher k/N (i.e

when spikes are generated by activation of a larger proportion of inputs). Note the different ranges for k/N in

upper and lower panels.

First spike latency depended on both the membrane time constant τ_l and the

reliability of the synaptic inputs k/N (Fig. 5A-D). All but the very fastest time constants

produced shorter latency spikes utilizing a rate code compared to a hybrid code, with

delays being reduced by up to 4.5 ms. Cells requiring fewer vesicles to spike benefit from

the wider temporal window of vesicle release in univesicular compared to multivesicular

events (as seen in Fig. 1F). However, the more reliable the inputs the weaker this effect

(Fig. 5D). At an intermediate range of k/N hybrid inputs generated spikes with shorter

latencies and then at higher k/N there was no dependence on coding strategy.

The general picture is that the rate code generates spikes with shorter latency only in

larger neurons in which spiking is driven by larger numbers of less reliable synaptic inputs

- conditions more likely to occur in brain regions such as the cortex than the retina or other

circuits with more reliable synapses.

510
MVR increases information transmission across a range of conditions

Having established that MVR impacts both spike count and timing we asked how these

effects interact to alter the transmission of information (Borst and Theunissen, 1999).

The mutual information was calculated between a set of nine stimuli (contrasts of 20%,

60% and 100% at frequencies of 5 Hz, 10 Hz and 15 Hz) and each of three measures of

the response in the model neuron: spike count, spike time and the total information within

the spike sequence. Supplementary Figure 2 shows the probability distributions of quanta

per event, P(Qe), and temporal jitter functions, TJ(Q), while Supplementary Figures 3 and

4 show responses to the stimulus of the example midget and peripheral cells in Fig. 3. A

neuron that encodes a total of $\log_2(9) = 3.17$ bits of information over a 200 ms time

window is discriminating perfectly between the nine stimuli.

Figure 6. Hybrid coding increased information in the spike output over a range of physiologically-relevant conditions

A. Left: heat map showing the information transmitted in the spike count generated by hybrid synaptic inputs for cells of varying k/N and τ_l. Mutual Information was averaged over values of k and N shown in Table 1 and was measured over a time-window of 200 ms. These values can therefore be multiplied by 5 to obtain information rates as bits s^{-1}. Middle: Mutual Information in spike timing. Right: the total Mutual Information representing the sum of count and timing information. The colour scale bar applies to all three maps. Maximum possible information was 3.17 bits. More information was contained in the spike count compared to spike times. **B.** As A, but for rate-coded synaptic inputs operating at the same average release rates. **C.** The difference between A and B (hybrid - rate). The colour scale (right) shows combinations of parameters in which hybrid inputs generated more spikes in green. Zero difference is white and combinations of parameters in which rate-coded inputs generated more spikes are in red. Note that there are some situations in which count information is favoured by rate-coded inputs while time information is favoured by hybrid inputs (and vice versa) but total information is favoured by hybrid inputs over a wider range of conditions (right). The parameters for the specific model cells featured in Fig. 3 are indicated as M (midget) and P (peripheral) in the heat plot for the difference in total information.

The heat plots in Fig. 6 demonstrate that spike count carried more of the total information than spike time for both the synaptic coding strategies. But the relative advantages of MVR and rate codes again depended on the time-constant of the target neuron and the reliability of the inputs driving spikes. In a cell of given time-constant, an

increase in the reliability of inputs caused the hybrid code to became more efficient at

generating spikes (Fig. 4) with shorter latency (Fig. 5) resulting in more information

transmission (Fig. 6). In the midget cell, for instance, the spike count over a 200 ms

period carried 0.07 bits more information when generated by hybrid inputs, while spike

time carried 0.08 bits more, and the total information difference was ~0.16 bits (equivalent

to an information rate of 0.82 bits s^{-1}). The largest difference in information rate in favour

of the hybrid code was 3.8 bits s^{-1} or 24% of the maximum possible information rate,

occurring when the post-synaptic cell required 25 vesicles to spike, had 250 inputs, and a

1 ms time constant.

The rate code carried marginally more of the total information only in lager cells in

which larger numbers of less reliable synapses converge. For the peripheral ("large")

RGC highlighted in Fig. 3, for instance, we calculated mutual information differences

(hybrid – rate) of -0.12 for spike count and 0.11 for spike time, yielding a total information

difference of -0.01 bits. The largest difference in information rate in favour of the rate

code was only 0.24 bits s^{-1}, occurring when only 10 vesicles were required to generate a

spike, with 50 inputs, and a time constant of 50 ms.

Together, the simulations in Figs. 2-6 indicate that synapses which generate MVR

can often trigger more spikes per released vesicle compared to a classical Poisson

synapse in which all vesicles are released independently. In cells with time-constants less

than 15 ms, the tendency for MVR to enhance the transmission of information becomes

greater as k/N falls below ~0.8. These conditions are physiologically relevant. In the

peripheral retina, for instance, alpha ganglion cells have membrane time-constants less

than 5 ms and ten or fewer quanta released from thousands of synapses are sufficient to

generate a spike (Freed and Sterling, 1988; O'Brien et al., 2002). More morphologically

compact neurons, such as midget ganglion cells in the fovea of primates, only receive

inputs from synapses from a single midget bipolar cell and are likely to have even shorter

time-constants (Sinha et al., 2017).

MVR increases the efficiency of information transmission across a range of conditions

Neurons can transmit more information by spiking at higher rates but this comes at a relatively large energetic cost (Laughlin, 2001). The release of vesicles and generation of spikes is the major consumer of energy in the brain with one estimate being of the order of ~24,000 ATP molecules consumed per bit of information transmitted (Attwell and Laughlin, 2001; Harris et al., 2012). The efficiency with which vesicles drive the spike code is therefore likely to have been an evolutionary constraint on the vesicle code itself (Sterling and Laughlin, 2015).

To investigate the potential effects of MVR on the efficiency of information transmission we normalized the measurements of total information summarized in Fig. 6A and B as bits per vesicle and bits per spike, as shown in Fig. 7A and B. Considering the amount of information per vesicle, the relative advantages of hybrid and rate codes can be seen to follow a clear pattern: the more reliably inputs responded (i.e the higher k/N) the broader the range of cell time-constants over which hybrid-coded inputs improved the efficiency with which vesicles transferred information through spikes in the target neuron (Fig. 7A right). The rate-code was only slightly advantageous in neurons acting as the best temporal integrators receiving the least reliably responding inputs. The highest vesicle efficiency using either synaptic code was ~0.044 bits per vesicle.

Figure 7. Hybrid coding increased the efficiency of information transmission over a range of conditions

A. Left: heat map showing the information transmitted per vesicle generated by hybrid synaptic inputs for cells of varying k/N and τ_l. Middle: the same for rate-coded synaptic inputs operating at the same average release rates. Right: The difference in the efficiency of information transmission considered as bits per vesicle (hybrid - rate). The colour scale (right) shows combinations of parameters in which hybrid inputs generated more spikes in green. The parameters for the specific model cells featured in Fig. 3 are indicated as M (midget) and P (peripheral) in the heat plot. **B.** As A, but considering efficiency as bits per spike. Note that the hybrid vesicle code increases the efficiency of information transmission across a range of conditions. The pure rate vesicle code was only advantageous in LIF neurons with the longest time-constants driven by the most reliably responding synaptic inputs.

A similar pattern was observed when we quantified the amount of information per spike: the more reliably inputs responded the broader the range of cell time-constants over which hybrid-coded inputs increased the amount of information per spike (Fig. 7B right). The highest spike efficiency was ~3 bits per spike. A comparison can be made with the information transmitted by spikes in RGCs responding to white-noise stimuli, where the most sluggish transmit ~3.5 bits/spike, while those that fire most briskly encode ~2 bits/spike (Koch et al., 2006). The results in Fig. 7 encapsulate hat we believe is the

most fundamental insight if this study – the potential of MVR to increase the efficiency with

which vesicles are used to transmit information.

The first synapse in hearing

MVR is also a prominent property of the ribbon synapse of auditory hair cells, where the

fusion of multiple vesicles can be synchronized on timescales as short as 100 µs (Fuchs

and Glowatzki, 2015; Glowatzki and Fuchs, 2002). This presents a special case because

there is no convergence onto the target, each Type I afferent fiber receiving sensing

glutamate released from just one ribbon synapse. This simplified situation allowed us to

use a modelling framework employing marked Poisson Processes (see Methods).

Experiments indicate that spikes in the afferent fiber can be triggered by just a few

vesicles and in some cases perhaps as a few as one (Grabner and Moser, 2018;

Rutherford et al., 2012). We therefore considered two broad situations:

i) $k = 1$. *Any* vesicular event, regardless of quantal content, is capable of generating a

spike.

ii) $k > 1$. Some (but not all) multivesicular events are capable of generating a spike from

rest.

The transmission of information was strongly dependent on both the number of

vesicles required to generate a spike, k, and the membrane time constant but again the

nature of this dependence differed for synapses employing a pure rate code compared to

those also employing MVR (Fig. 8A). Rate coding produced the maximum mutual

information in the simulations when $k = 1$, where the spike sequence in the afferent

reproduced the vesicle sequence leaving the synapse (Fig. 7A, red). In this situation a

multivesicular event is no more effective than a univesicular event so the hybrid code

produces fewer spikes per vesicle and reduces the efficiency of information transmission

(Fig. 8A, black).

Figure 8. Spike Count Information for Amplitude (black) and Rate (red) inputs as a function of τ_l and k where N = 1. A. Mutual information for the rate input (dash) and amplitude input (solid) as a function of the vesicles sufficient to generate a spike. Values shown for τ_l of 50, 20, 10, and 1 ms. **B**. Mutual information difference (hybrid – rate) for the data shown in A. **C**. Mutual information (as **A**) in matrix form. **D**. Mutual information difference in matrix form.

As the gain of synaptic transmission decreased and more vesicles were required to generate a spike (k > 1), the picture began to change. Increasing k reduced the spike count and effectively abolished spiking at k > 3 when tau = 1 ms (Fig. 8A and B). Essentially, this is because the very short time-constant of the target neuron (mimicking an afferent fiber) did not allow for effective summation of vesicles. Hybrid coding, however, expanded the range of responses by increasing the number of spikes a stimulus could generate, maximizing at a value when most events at higher contrast individually generated a spike (approximately k = 4 for this range of conditions, as seen in Fig. 8B and D). This switch in the relative efficiency of the two synaptic coding strategies starkly illustrates a key functional advantage of the hybrid code: presynaptic integration of

vesicles by MVR compensates for situations where the integration time of the post-
synaptic neuron is short and limits summation post-synaptically.

The heatmap in Fig. 8D demonstrates that the increase in the efficiency of information
transmission caused by MVR was most dramatic in a target neuron with time-constants
less than about 10-15 ms in which a spike could be triggered by the arrival of 3-5 vesicles.
For $5 < k < 10$, MVR still utilized vesicles more efficiently than a pure rate-code (Fig. 8D),
despite the fact that not all MVR events were capable of generating a spike even at the
highest contrasts. MVR in rat hair cells can generate events equivalent to up to ~22
vesicles (Glowatzki and Fuchs, 2002) suggesting that the advantages of a hybrid code
might be exerted over a broad range of k in the auditory system.

Discussion

The question motivating this study was "why MVR?" and the results indicate that the
answer is "because it can increase the efficiency with vesicles are used to transmit
information".

A number of studies have used leaky integrate-and-fire models to investigate the
relationship between vesicle release, spikes and information, usually treating synapses as
Poisson machines in which vesicles are released independently (de la Rocha et al., 2002;
Goldman, 2004; London et al., 2010; Zador, 1998). But this assumption does not hold at
many synapses exhibiting MVR (Auger et al., 1998; Glowatzki and Fuchs, 2002; Hays et
al., 2021; Singer et al., 2004) and here we have shown that over a range of conditions
mimicking transmission of visual signals to retinal ganglion cells of different sizes,
presynaptic integration of vesicles by MVR increased the efficiency of spike generation
compared to a simple rate-code in which all vesicles were released independently (Figs.
4, 6-7). In the special case of a single synaptic input, as occurs where auditory hair cells
drive afferent fibers, MVR increased the efficiency of information transfer whenever spike
generation required depolarization greater than that caused by a single vesicle (Fig. 8).
We identified two aspects of the process driving spikes that interact to determine the

relative efficiency of a pure rate-code compared to a hybrid code: the time-constant of the

target neuron and the reliability of the synaptic inputs. MVR tended to be advantageous

when i) the neurons time-constant was shorter, causing less post-synaptic summation of

synaptic potentials at physiological rates of vesicle release, and ii) individual synaptic

inputs were more reliable so that a lower degree of convergence was required to

depolarize the target to threshold for a given stimulus strength.

Drawbacks of a pure rate code

It is clear that neurons represent sensory stimuli, at least in part, using a simple rate-code,

where information is contained in the number of spikes over a given time-window (Rieke

and Warland, 1999). But it has long been recognized that a potential drawback of a

simple rate-code is the time-scale on which it can transmit information: the more variable

a neural response to a stimulus the longer the observation time required to detect it to a

given degree of certainty (Gerstner et al., 1997; Stein et al., 2005). At the ribbon synapse

of bipolar cells, for instance, the maximum sensitivity to changes in contrast occurs

around average release rate $R = 20$ vesicles s^{-1} and a 10% increase in contrast increases

release by a factor of $a = 1.8$ (James et al., 2019). If release events are Poisson

distributed, signal detection theory can be used to quantify the time-window over which

the response would need to be observed to differentiate it from ongoing release: a SNR of

2 would require counting an extra 14 vesicles over an observation time (Δt) of ~0.9 s

(equations 7-9 in Methods). But vision operates more rapidly. Our visual system can

process a scene in less than 150 ms (Thorpe et al., 1996) and neurons in the cortex of

monkeys can respond to images changing at intervals as short as 14 ms (Keysers et al.,

2001).

One feature of the retinal circuit that will shorten the time-scale of information

transmission using a rate-code is convergence of bipolar cell synapses onto RGCs. N

equivalent Poisson inputs allows a given SNR to be achieved with a time-window that

varies as $1/\sqrt{N}$ (Faisal et al., 2008; Gerstner et al., 1997; Rusakov et al., 2020).

Continuing with the example above and considering a time-window of 100 ms, the output

of 50 synapses is would provide a SNR of 2 in a time-window of 100 ms, but at the cost of

$N*(1-a)*R*\Delta t = 80$ extra vesicles. Although faster, this still seems costly.

Encoding discrete visual events

The discussion of potential problems with a pure rate code is closely linked to the idea

that the firing rate of a neuron or release rate of a synapse encodes the sensory variable

continuously. In fact, if a varying stimulus is applied, most RGCs fire in bursts from rest,

driven by fusillades of vesicles released from bipolar cells (Berry et al., 1997b; Freed,

2005; Keat et al., 2001). The information that RGCs convey is therefore represented not

just by the spike count but also by the precise timing of spikes (Gutig et al., 2013; Meister

et al., 1995; Victor, 2000) and it has been shown that such a temporal coding strategy can

significantly improve the speed of information transmission (Butts et al., 2007; Gollisch

and Meister, 2008). Focusing on an individual active zone using iGluSnFr reveals that

these also signal visual events in bursts, including MVR events of varying amplitude (Fig.

1A and C).

In considering different synaptic coding strategies it might therefore be more helpful to

focus on the representation of temporally discrete events rather than the value of a

continuous variable such as contrast. It has been suggested that the onset of a burst in

an RGC provides information about when a visual event occurs, while the number of

spikes within the burst represent properties such as its magnitude (Keat et al., 2001). The

temporal jitter in thr first spike within a burst can be as low as a few milliseconds (Berry et

al., 1997a; Freed, 2005) and it is notable that larger MVR events from bipolar cells

achieve a similar temporal precision (Fig. 1E and F).

This comparison of the vesicle code in bipolar cells and the spike code in post-

synaptic RGCs highlights one of the potential advantages of representing a stimulus using

synaptic symbols of different amplitude: an unexpected symbol immediately imparts new

information and larger MVR events that are more likely to trigger a spike are indeed rarer

(Fig. 1C) (James et al., 2019). Our analysis of mutual information was more concerned

with the "what" of the stimulus (contrast), and spike count carried more of the total

information than spike time for either of the synaptic coding strategies (Fig. 7).   This

feature of the results might, however, represent limitations of the LIF model, in which we

only considered excitation.   The precise timing of spikes in RGCs is also dependent on

inhibitory inputs, especially feedforward inhibition that increases the temporal precision of

spikes and, crucially, also causes spikes to be fired in bursts (Johnston and Lagnado,

2015; Murphy-Baum and Taylor, 2018).   Network models incorporating a wider range of

biophysical parameters will help us understand how excitation and inhibition interact to

determine the temporal precision of the spike code leaving the retina.

Encoding auditory events

The spike code carrying auditory information in cochlear afferents is determined only by

excitatory inputs from hair cells and is therefore likely to reflect the temporal precision of

ribbon synapses more directly than the spike code leaving the retina. The synaptic output

from hair cells has been measured *in vitro* with electrophysiological precision where it is

found that larger MVR events are more tightly phase-locked to a sinusoidal voltage-clamp

stimulus (Li et al., 2014). Notably, MVR events in hair cells can be as large as ~20 vesicle

equivalents when triggered using electrophysiology (Glowatzki and Fuchs, 2002) but it is

unclear if these can also be triggered by sound. Here we used the statistics of MVR

measured in bipolar cells *in vivo*, where the largest events evoked by the highest

contrasts are composed of 9-11 vesicles (James et al., 2019). A better understanding of

how the ribbon synapse of hair cells drive the spke code in auditory fibers will require

experimental measurements of the statistics of vesicle release in response to sounds of

different intensities and frequencies in hair cells with different characteristic frequencies.

Future directions

To put the statistics of vesicle release into a functional context we also need an understanding of the spike code that it drives. A key next step will be to obtain direct experimental measurements of how effectively MVR events of different size trigger spikes. This will likely vary according to the time-constant of the RGC and the number and strength of it's inputs, which in turn will vary according to the functional class it belongs and its location in the retina. In the peripheral retina, for instance, alpha ganglion cells have membrane time-constants less than 5 ms and on average ten quanta are released from thousands of synapses for each spike generated (Freed, 2005). More morphologically compact neurons, such as midget ganglion cells in the fovea of primates, only receive inputs from a single midget bipolar cell and are likely to have even shorter time-constants (Sinha et al., 2017). The simpler organization of the first stage in hearing, where spikes in afferents are driven by a single synapse, provides a beautiful context in which to investigate how the vesicle code determines the spike code transmitting sensory information.

References

Abbott, L.F. (1999). Lapicque's introduction of the integrate-and-fire model neuron (1907). Brain Res Bull *50*, 303-304.

Allen, C., and Stevens, C.F. (1994). An evaluation of causes for unreliability of synaptic transmission. Proceedings of the National Academy of Sciences *91*, 10380-10383.

Attwell, D., and Laughlin, S.B. (2001). An energy budget for signaling in the grey matter of the brain. Journal of Cerebral Blood Flow & Metabolism *21*, 1133-1145.

Auger, C., Kondo, S., and Marty, A. (1998). Multivesicular release at single functional synaptic sites in cerebellar stellate and basket cells. J Neurosci *18*, 4532-4547.

Baden, T., Esposti, F., Nikolaev, A., and Lagnado, L. (2011). Spikes in retinal bipolar cells phase-lock to visual stimuli with millisecond precision. Curr Biol *21*, 1859-1869.

Berry, M.J., Warland, D.K., and Meister, M. (1997a). The structure and precision of retinal spike trains. Proceedings of the National Academy of Sciences *94*, 5411-5416.

Berry, M.J., Warland, D.K., and Meister, M. (1997b). The structure and precision of retinal spike trains. Proc Natl Acad Sci U S A *94*, 5411-5416.

Borst, A., and Theunissen, F.E. (1999). Information theory and neural coding. Nat Neurosci *2*, 947-957.

Branco, T., and Staras, K. (2009). The probability of neurotransmitter release: variability and feedback control at single synapses. Nat Rev Neurosci *10*, 373-383.

Buracas, G.T., Zador, A.M., DeWeese, M.R., and Albright, T.D. (1998). Efficient discrimination of temporal patterns by motion-sensitive neurons in primate visual cortex. Neuron *20*, 959-969.

Burkitt, A.N. (2006a). A review of the integrate-and-fire neuron model: I. Homogeneous synaptic input. Biol Cybern *95*, 1-19.

Burkitt, A.N. (2006b). A review of the integrate-and-fire neuron model: II. Inhomogeneous synaptic input and network properties. Biol Cybern *95*, 97-112.

Butts, D.A., Weng, C., Jin, J., Alonso, J.M., and Paninski, L. (2011). Temporal precision in the visual pathway through the interplay of excitation and stimulus-driven suppression. J Neurosci *31*, 11313-11327.

Butts, D.A., Weng, C., Jin, J., Yeh, C.-I., Lesica, N.A., Alonso, J.-M., and Stanley, G.B. (2007). Temporal precision in the neural code and the timescales of natural vision. Nature *449*, 92-95.

Calkins, D.J., Schein, S.J., Tsukamoto, Y., and Sterling, P. (1994). M and L cones in macaque fovea connect to midget ganglion cells by different numbers of excitatory synapses. Nature *371*, 70-72.

Carleton, A., Accolla, R., and Simon, S.A. (2010). Coding in the mammalian gustatory system. Trends Neurosci *33*, 326-334.

Christie, J.M., and Jahr, C.E. (2006). Multivesicular release at Schaffer collateral-CA1 hippocampal synapses. J Neurosci *26*, 210-216.

de la Rocha, J., Nevado, A., and Parga, N. (2002). Information transmission by stochastic synapses with short-term depression: neural coding and optimization. Neurocomputing *44*, 85-90.

Destexhe, A., and Rudolph, M. (2004). Extracting Information from the Power Spectrum of Synaptic Noise. Journal of Computational Neuroscience *17*, 327-345.

Faisal, A.A., Selen, L.P., and Wolpert, D.M. (2008). Noise in the nervous system. Nat Rev Neurosci *9*, 292-303.

Freed, M.A. (2005). Quantal encoding of information in a retinal ganglion cell. J Neurophysiol *94*, 1048-1056.

Freed, M.A., and Sterling, P. (1988). The ON-alpha ganglion cell of the cat retina and its presynaptic cell types. J Neurosci *8*, 2303-2320.

Fuchs, P.A., and Glowatzki, E. (2015). Synaptic studies inform the functional diversity of cochlear afferents. Hear Res *330*, 18-25.

Gerstner, W., Kreiter, A.K., Markram, H., and Herz, A.V. (1997). Neural codes: firing rates and beyond. Proc Natl Acad Sci U S A *94*, 12740-12741.

Glowatzki, E., and Fuchs, P.A. (2002). Transmitter release at the hair cell ribbon synapse. Nat Neurosci *5*, 147-154.

Goldberg, J.M., and Brown, P.B. (1969). Response of binaural neurons of dog superior olivary complex to dichotic tonal stimuli: some physiological mechanisms of sound localization. J Neurophysiol *32*, 613-636.

Goldman, M.S. (2004). Enhancement of information transmission efficiency by synaptic failures. Neural computation *16*, 1137-1162.

Gollisch, T., and Meister, M. (2008). Rapid neural coding in the retina with relative spike latencies. Science *319*, 1108-1111.

Gollisch, T., and Meister, M. (2010). Eye smarter than scientists believed: neural computations in circuits of the retina. Neuron *65*, 150-164.

Grabner, C.P., and Moser, T. (2018). Individual synaptic vesicles mediate stimulated exocytosis from cochlear inner hair cells. Proc Natl Acad Sci U S A *115*, 12811-12816.

Harris, Julia J., Jolivet, R., and Attwell, D. (2012). Synaptic Energy Use and Supply. Neuron *75*,
762-777.

Hays, C., Sladek, A., Field, G., and Thoreson, W. (2021). Properties of multi-vesicular release from
mouse rod photoreceptors support transmission of single photon responses. eLife *10*.

Holler, S., Kostinger, G., Martin, K.A.C., Schuhknecht, G.F.P., and Stratford, K.J. (2021). Structure
and function of a neocortical synapse. Nature *591*, 111-116.

Huang, C.H., Bao, J., and Sakaba, T. (2010). Multivesicular release differentiates the reliability of
synaptic transmission between the visual cortex and the somatosensory cortex. J Neurosci *30*,
11994-12004.

Jacoby, R.A., Wiechmann, A.F., Amara, S.G., Leighton, B.H., and Marshak, D.W. (2000). Diffuse
bipolar cells provide input to OFF parasol ganglion cells in the macaque retina. J Comp Neurol *416*,
6-18.

James, B., Darnet, L., Moya-Diaz, J., Seibel, S.H., and Lagnado, L. (2019). An amplitude code
transmits information at a visual synapse. Nat Neurosci *22*, 1140-1147.

Johnson, D.H. (1996). Point process models of single-neuron discharges. J Comput Neurosci *3*,
275-299.

Johnston, J., and Lagnado, L. (2015). General features of the retinal connectome determine the
computation of motion anticipation. eLife *4*, e06250.

Kaplan, E., and Shapley, R.M. (1986). The primate retina contains two types of ganglion cells, with
high and low contrast sensitivity. Proc Natl Acad Sci U S A *83*, 2755-2757.

Kayser, C., Montemurro, M.A., Logothetis, N.K., and Panzeri, S. (2009). Spike-Phase Coding
Boosts and Stabilizes Information Carried by Spatial and Temporal Spike Patterns. Neuron *61*,
597-608.

Keat, J., Reinagel, P., Reid, R.C., and Meister, M. (2001). Predicting Every Spike: A Model for the
Responses of Visual Neurons. Neuron *30*, 803-817.

Keysers, C., Xiao, D.-K., Földiák, P., and Perrett, D.I. (2001). The speed of sight. Journal of
cognitive neuroscience *13*, 90-101.

Koch, K., McLean, J., Segev, R., Freed, M.A., Berry, M.J., 2nd, Balasubramanian, V., and Sterling,
P. (2006). How much the eye tells the brain. Curr Biol *16*, 1428-1434.

Kolb, H., and Marshak, D. (2003). The midget pathways of the primate retina. Doc Ophthalmol *106*,
67-81.

Lagnado, L., and Schmitz, F. (2015). Ribbon Synapses and Visual Processing in the Retina. Annu
Rev Vis Sci *1*, 235-262.

Laughlin, S.B. (2001). Energy as a constraint on the coding and processing of sensory information.
Curr Opin Neurobiol *11*, 475-480.

Li, G.L., Cho, S., and von Gersdorff, H. (2014). Phase-locking precision is enhanced by
multiquantal release at an auditory hair cell ribbon synapse. Neuron *83*, 1404-1417.

Lisman, J.E., Raghavachari, S., and Tsien, R.W. (2007). The sequence of events that underlie
quantal transmission at central glutamatergic synapses. Nat Rev Neurosci *8*, 597-609.

London, M., Roth, A., Beeren, L., Hausser, M., and Latham, P.E. (2010). Sensitivity to
perturbations in vivo implies high noise and suggests rate coding in cortex. Nature *466*, 123-127.

Manwani, A., and Koch, C. (2001). Detecting and estimating signals over noisy and unreliable
synapses: information-theoretic analysis. Neural Comput *13*, 1-33.

Moreno-Bote, R. (2014). Poisson-like spiking in circuits with probabilistic synapses. PLoS
computational biology *10*, e1003522-e1003522.

Murphy-Baum, B.L., and Taylor, W.R. (2018). Diverse inhibitory and excitatory mechanisms shape
temporal tuning in transient OFF α ganglion cells in the rabbit retina. The Journal of physiology
596, 477-495.

Neves, G., and Lagnado, L. (1999). The kinetics of exocytosis and endocytosis in the synaptic
terminal of goldfish retinal bipolar cells. J Physiol *515 (Pt 1)*, 181-202.

O'Brien, B.J., Isayama, T., Richardson, R., and Berson, D.M. (2002). Intrinsic physiological
properties of cat retinal ganglion cells. J Physiol *538*, 787-802.

Panzeri, S., Senatore, R., Montemurro, M.A., and Petersen, R.S. (2007). Correcting for the
sampling bias problem in spike train information measures. J Neurophysiol *98*, 1064-1072.

Pillow, J.W., Paninski, L., Uzzell, V.J., Simoncelli, E.P., and Chichilnisky, E.J. (2005). Prediction
and decoding of retinal ganglion cell responses with a probabilistic spiking model. J Neurosci *25*,
11003-11013.

Quian Quiroga, R., and Panzeri, S. (2009). Extracting information from neuronal populations:
information theory and decoding approaches. Nat Rev Neurosci *10*, 173-185.

Reinagel, P., and Reid, R.C. (2002). Precise firing events are conserved across neurons. J
Neurosci *22*, 6837-6841.

Rieke, F., and Warland, D. (1999). Spikes: exploring the neural code (MIT press).

Rusakov, D.A., Savtchenko, L.P., and Latham, P.E. (2020). Noisy Synaptic Conductance: Bug or a
Feature? Trends Neurosci *43*, 363-372.

Rutherford, M.A., Chapochnikov, N.M., and Moser, T. (2012). Spike encoding of neurotransmitter
release timing by spiral ganglion neurons of the cochlea. J Neurosci *32*, 4773-4789.

Schwartz, O., Pillow, J.W., Rust, N.C., and Simoncelli, E.P. (2006). Spike-triggered neural
characterization. J Vis *6*, 484-507.

Shannon, C. (1948). A Mathematical Theory of Communication. Bell System Technical Journal *27*,
379-423.

Singer, J.H., Lassova, L., Vardi, N., and Diamond, J.S. (2004). Coordinated multivesicular release
at a mammalian ribbon synapse. Nat Neurosci *7*, 826-833.

Sinha, R., Hoon, M., Baudin, J., Okawa, H., Wong, R.O.L., and Rieke, F. (2017). Cellular and
Circuit Mechanisms Shaping the Perceptual Properties of the Primate Fovea. Cell *168*, 413-
426.e412.

Smetters, D.K., and Zador, A. (1996). Synaptic transmission: Noisy synapses and noisy neurons.
Current Biology *6*, 1217-1218.

Stein, R.B., Gossen, E.R., and Jones, K.E. (2005). Neuronal variability: noise or part of the signal?
Nature Reviews Neuroscience *6*, 389-397.

Sterling, P., and Laughlin, S. (2015). Principles of neural design (MIT press).

Thorpe, S., Fize, D., and Marlot, C. (1996). Speed of processing in the human visual system.
Nature *381*, 520-522.

Uzzell, V.J., and Chichilnisky, E.J. (2004). Precision of spike trains in primate retinal ganglion cells.
J Neurophysiol *92*, 780-789.

Victor, J.D. (2006). Approaches to Information-Theoretic Analysis of Neural Activity. Biol Theory *1*,
302-316.

Zador, A. (1998). Impact of synaptic unreliability on the information transmitted by spiking neurons.
J Neurophysiol *79*, 1219-1229.

 Supplementary Information

940 **Supplementary Figure 1**

944 **Supplementary Figure 1. Graphical description of Poisson Splitting.** Left: a Poisson

945 Process (PPs) is split dependent upon time, yielding independent PPs, where the total

946 release can then be summed. Right: Time dependent splitting function used for the

947 simulations.

Supplementary Figure 2

Supplementary Figure 2. Temporal Jitter functions (TJ(Q)) and Probability Mass Functions

(P(Qe)) for all 9 stimuli used for the computation of mutual information. Note that increasing

contrast increases shifts the distribution of quanta per event (P(Qe)) towards higher values and

decreases the temporal jitter, while increasing the stimulus frequency shifts the distribution of

quanta per event towards lower values and decreases temporal jitter.

Supplementary Figure 3

Supplementary Figure 3. Responses of the example "midget" cell to the stimulus set used

in information theory calculations.

A. Raster plots for hybrid coded synaptic inputs at the frequency and contrast indicated. This was

a "midget" cell simulated with: inputs = 50, k = 10, τ_l = 5 ms, v_e = 0, θ = -50 mV, v_{rest} = -70 mV.

The number of vesicles required to generate a spike (k) was 10. These are the same parameters

as the example cell featured in Fig. 3A-E. **B.** Same as **A**, but for purely rate-coded synaptic inputs

in which all vesicles were released independently.

Supplementary Figure 4

Supplementary Figure 4. Responses of the example "peripheral" cell to the stimulus set

used in information theory calculations.

A. Raster plots for hybrid coded synaptic inputs at the frequency and contrast indicated. This was

a "peripheral" cell simulated with: inputs = 500, k = 100, τ_l = 50 ms, v_e = 0, θ = -50 mV, v_{rest} = -70

mV, k = 100. These are the same parameters as the example cell featured in Fig. 3F-J. **B.** Same

as **A**, but for purely rate-coded synaptic inputs in which all vesicles were released independently.