Brain state and cortical layer-specific mechanisms underlying perception at threshold

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ABSTRACT

Identical stimuli can be perceived or go unnoticed across successive presentations, producing divergent behavioral outcomes despite similarities in sensory input. We sought to understand how fluctuations in behavioral state and in cortical layer and cell-class specific neural activity underlie this perceptual variability. We analyzed physiological measurements of state and laminar electrophysiological activity in visual area V4 while monkeys were rewarded for correctly reporting a stimulus change at perceptual threshold. We find that hit trials are characterized by a behavioral state with increased arousal and improved eye position stability. During hit trials, target stimuli evoke stronger responses in V4, and excitatory neurons in the superficial layers, the primary feed-forward output of the cortical column, exhibit lower variability. Hit trials are characterized by greater synchrony between the output layers of the cortex during spontaneous activity, while the stimulus evoked period shows elevated synchrony in the feed-forward pathway. Taken together, these results suggest that a state of elevated arousal and stable retinal images allow enhanced processing of sensory stimuli, which contributes to hits at perceptual threshold.

INTRODUCTION

Physical properties of stimuli strongly influence perception. Low intensity stimuli are detected infrequently. As intensity increases, detection probability remains low until some perceptual threshold is crossed, after which stimuli are perceived robustly. A psychometric function (1-3) mathematically describes this property of perception. Only within a narrow range around the perceptual threshold do stimuli lead to significant trial-to-trial perceptual variance. While many studies present stimuli at threshold (4-7), few have probed the laminar cortical microcircuit mechanisms that underlie successful or unsuccessful perception under these conditions (8, 9).

Prior studies have characterized how perceived stimuli trigger stronger information propagation from earlier visual areas to higher order visual and frontal regions (4, 9). Information propagation and sensory processing are strongly influenced by brain states such as arousal and attention (8, 10). Arousal has long been known to modulate cortical activity (11-13) and impact behavioral performance on a variety of sensory tasks (14-16). Activity in visual area V4, a critical intermediate region in the ventral visual processing stream (17-19) is known to be strongly modulated by attention (20-23). Attention enhances the firing rates of V4 neurons, increases the reliability in firing of individual neurons, and decreases correlated fluctuations among pairs of neurons (21, 24-26). Brain state dynamics influence both cortical and subcortical structures while contributing to behavior (27, 28). On and off state dynamics in V4 ensembles have been hypothesized to reflect fluctuations in attention and have been shown to correlate with behavioral performance (29, 30).

The visual cortex has a columnar architecture in which multiple cell classes (31-

35) across the cortical layers (18, 36) form distinct sub-populations. These sub-populations have unique and stereotyped patterns of connectivity, thus forming a canonical microcircuit that orchestrates the encoding and flow of information (37, 38). Moreover, these sub-populations contribute uniquely to sensory processing and are differentially modulated by brain states (25, 39-41). While it has been shown that attentional modulation varies across cortical layers (39, 41-47), the role of these sub-populations in attentive perception at threshold remains poorly understood. Moreover, the influence of physiological states, that may be responsible for different outcomes at threshold, on these sub-populations has not been studied in detail.

Here we examine the neural mechanisms that regulate perception at threshold. We specifically focus on the columnar microcircuit mechanisms within area V4. We hypothesized that minor fluctuations in behavioral state, such as arousal and visual sensitivity, and in the activity of neural sub-populations across the layers of the visual cortex, result in different perceptual outcomes at threshold. Specifically, we hypothesized the output layers (II-III, V-VI) that project to higher cortical areas and subcortical structures would show signs of improved capacity for stimulus representation. We also hypothesized that improved information propagation throughout a cortical column would characterize successful perception at threshold. We find that differences in behavioral and lamina-specific neural states characterize correct and incorrect trials at threshold and explain perceptual variability.

RESULTS

To study the neural dynamics responsible for determining whether a stimulus presented

at perceptual threshold is perceived, we analyzed behavioral and cortical layer-specific neural data from area V4, collected while monkeys performed a cued attention task (39). Monkeys were trained to detect an orientation change in one of two Gabor stimuli that were presented concurrently at two spatial locations, and to report having seen the change by making an eye movement to the changed stimulus. Prior to a block of trials, monkeys were cued as to which of the two spatial locations was likely to undergo the orientation change (95% valid cue; presented at the start of each block). During a trial, “non-target” stimuli at a fixed reference orientation were repeatedly presented. Non-targets were turned on for 200ms at the two spatial locations, and then turned off for a variable interval (200-400ms). At a random time (1-5s, mean 3s) a “target” stimulus, differing in orientation from the non-targets, was presented at one of the locations. If the monkey reported having detected the orientation change by making an eye movement to the location of the target stimulus, it received a juice reward (Figure 1A, “hit” trial). If the monkey failed to detect the orientation change and instead continued to maintain fixation on the center of the monitor, it was not rewarded (Figure 1A, “miss” trial). In this study, we focused exclusively on trials in which the target stimulus was presented at the cued location (95% of trials). All figures relate exclusively to trials in which the change occurred at the cued location.

On each trial, the magnitude of the orientation change was drawn from a distribution that spanned multiple levels of difficulty. We fit the behavioral data with a logistic function (1) and defined the threshold condition as the orientation change that was closest to the 50% threshold of the fitted psychometric function for that session (Figure 1B, Experimental Procedures). We selected this subset of trials for further analysis, since

99 the constant target stimuli in these trials were equally likely to be perceived or not
100 perceived.

101 While monkeys performed this task, single- and multi-unit activity and local field
102 potentials (LFPs) were recorded in area V4 using 16-channel linear array electrodes
103 (Plexon inc., Figure 1-figure supplement 1A-E). The array was inserted perpendicular to
104 the cortical surface and spanned the cortical layers. We used current source density
105 (CSD) analysis (48) to estimate the boundaries between the superficial (I-III), input (IV),
106 and deep (V-VI) cortical layers (Figure 1-figure supplement 1E-F), and assign individual
107 neurons their layer identity (39). Single units were classified as either broad-spiking
108 (putative excitatory neurons) or narrow-spiking (putative inhibitory neurons) on the basis
109 of their waveform width using previously published techniques (peak to trough duration;
110 Figure 1-figure supplement 1D; see Methods; 31, 39, 40, 49, 50). Eye position and pupil
111 diameter were also recorded (ISCAN ETL-200). When analyzing pupil diameter and eye
112 position data, we considered all trials in the threshold condition in which the change
113 occurred at the cued location, regardless of whether the cued location was within the
114 receptive field of the recorded neurons. For all electrophysiological analyses, we only
115 considered trials in which the cued stimulus was within the receptive field of the recorded
116 neurons, and the stimulus change occurred at the cued location.

117 To assess the behavioral impact of variations in arousal and retinal image stability
118 across trials at the threshold condition, we compared pupil diameter and microsaccade
119 incidence across trail outcomes. Larger pupil diameter is thought to be a proxy for
120 elevated alertness and arousal (8, 14, 15, 51-54). We found that hit trials were associated
121 with larger pupil diameters compared to miss trials, both before and during non-target and

target stimulus presentations (Figure 2A). We quantified this difference in the estimation statistics framework (55, 56) by comparing effect sizes and using bootstrapping to estimate uncertainty in the differences. We found that the mean of the distribution of pupil diameters associated with hit trials is greater than that associated with misses (Figure 2B; complementary null hypothesis testing results in Table 1). Prior work has shown that the optimal state for sensory performance occurs at intermediate levels of arousal, with states of low and hyper arousal associated with decreased performance (14-16, 57-60). In both hit and miss trials, the mean pupil diameter was close to the optimal arousal state for perceptual performance (Figure 2C; 15). The average differences in pupil diameter across hit and miss trials reflect differences within the optimal state of intermediate arousal. Our results thus suggest that hits are more likely to occur during periods of greater arousal.

Microsaccades, small fixational eye movements of <1° in amplitude that occur during normal fixation, are associated with periods of decreased visual sensitivity due to unstable retinal images (61, 62). Microsaccades have been linked to suppressed neural responses in visual areas during perceptual tasks, impairing fine visual discrimination and behavioral performance (63, 64). We grouped trials in the threshold condition based on whether a microsaccade occurred in a 400ms window preceding the onset of the target stimulus. Most trials with a pre-target microsaccade were misses, whereas the majority of trials without a microsaccade in this window were hits (Figure 2D). There is a strong link between microsaccade direction and attention deployment (65-71). Consistent with previous reports we also find that microsaccades toward the attended stimulus were overrepresented in correct trials (Figure 2-figure supplement 1A, upper left). Conversely, microsaccades towards the attended stimulus were underrepresented in incorrect trials

(Figure 2-figure supplement 1A, lower left). There was a very low but statistically significant negative correlation between pupil diameter and microsaccade rate (Figure 2-figure supplement 1B, $r^2 = 0.006, p < 0.001$). Microsaccade rates and inter-microsaccade times are reported in Figure 2-figure supplement 1C-D. Overall, these results suggest that successful trials at threshold are significantly more likely to occur during a state of greater arousal and improved visual sensitivity.

Having established that hit trials are more likely to occur in states of elevated arousal and visual stability, we investigated whether hits are characterized by differential information processing in V4. Elevated stimulus-evoked firing rates in hits would indicate a stronger representation of the stimulus that could be necessary for accurate discrimination. We compared the firing rates of all neurons (single and multi-units) recorded in each cortical layer across hit and miss trials. For non-target stimuli, firing rates were equivalent for hits and misses in both the pre-stimulus (0-200ms before stimulus onset) and stimulus-evoked (60-260ms following stimulus onset) periods (Figure 3A). For the target stimulus, firing rates were once again equivalent in the pre-stimulus period, but hit trials were characterized by elevated firing across cortical layers in the stimulus-evoked period (Figure 3B-C). Broad and narrow-spiking neurons in both the input and deep layers respond more to target stimuli in hit trials, and trend towards elevated firing rates in the superficial layers during hits (Figure 3D). The average firing rate in response to target stimuli for each neuron is shown in Figure 3-figure supplement 1A for both hit and miss trials. It is important to note that the stimuli presented to the animals were identical for both hits and misses. Moreover, the responses to the target stimuli occur early, and elevated firing in hits emerges at the time of expected V4 response latencies

168 (70-100 ms; Figure 3-figure supplement 1C), and thus cannot be attributed to elevated
169 levels of firing due to subsequent saccade planning in these trials (Figure 3-figure
170 supplement 1B; expected >200ms; 72).

171 Variability in response reflects how reliably information is encoded by a neural
172 population. Lower baseline variability can enhance the ability of neurons to encode
173 stimulus differences. We calculated the Fano factor, a mean-normalized measure of trial-
174 to-trial variability in firing, for single-units in our population (Figure 4A). We find that broad-
175 spiking units in the superficial layer exhibited lower Fano factor during the pre-stimulus
176 period in hit trials (0-60ms before non-target stimulus onset, Figure 4B), indicating this
177 population of neurons fired more reliably when the animal correctly detected the
178 orientation change. This was not the case for broad-spiking neurons in other layers
179 (Figure 4B) or narrow-spiking neurons (Figure 4-figure supplement 1).

180 We next wanted to test how the relationship between spiking activity and LFPs
181 may differ across hits and misses. Spike-LFP synchrony can reflect cortical processing
182 and both within- and inter-areal coordination (73-75). We calculated the PPC (76), a
183 frequency resolved measure of spike-LFP phase-locking, for single and multi-units
184 relative to their local LFP signal during the pre-stimulus period (0-200ms before non-
185 target stimulus onset, Figure 5A). We averaged PPC values at low (3-12Hz), medium (15-
186 25Hz), and high (30-80Hz) frequency bands (superficial & Input: Figure 5-figure
187 supplement 1A-B; deep: Figure 5B & Figure 5-figure supplement 1C). Deep layer neurons
188 exhibit reduced low-frequency phase-locking in hit trials than in misses (Figure 5B),
189 suggesting an improvement in pooled signal-to-noise among this neural population.

190 Our results at the individual neuron or neural-sub-population levels suggest

191 enhanced processing of perceived stimuli. However, it is the concerted activity among
192 neural sub-populations that ultimately determine information flow through the laminar
193 cortical circuit. We therefore examined differences in interlaminar synchrony as
194 signatures of differential information flow between hit and miss trials. Spike-spike
195 coherence (SSC) is a frequency resolved measure of the degree to which two spike trains
196 fluctuate together (26, 77). We measured interlaminar SSC for spike trains from pairs of
197 cortical layers, each spike train being comprised of all recorded action potentials in a
198 given layer (See Methods). We computed interlaminar SSC separately for hit and mis
199 trials in both the pre-stimulus (0-200ms before non-target stimulus onset, Figure 6A) and
200 non-target stimulus-evoked (60-260ms after non-target stimulus onset, Figure 7A)
201 periods, matching the firing rates across hit and miss trials separately for the pre-stimulus
202 and non-target stimulus-evoked conditions. We averaged SSC for each pair of layers
203 across three frequency bands, 3-12Hz, 15-25Hz, and 30-80Hz (Figure 6B and 7B).
204 Overall, hit trials have greater interlaminar SSC compared to misses at almost all
205 frequencies (Figure 6B and 7B). In the pre-stimulus period, the strongest SSC difference
206 between hits and misses was observed between the superficial and deep layers across
207 all frequencies (Figure 6B, middle panel). This implies greater synchrony of the output
208 layers of the cortex during hit trials. In contrast, this pattern was directionally the same
209 during the non-target stimulus-evoked period, but stronger in the other layer pairs, with
210 greater SSC differences being found in pairs that involve the input layer (Figure 7B, top
211 and bottom). This may reflect a higher degree of stimulus-driven feed-forward information
212 propagation during hit trials. When comparing across time (pre-stimulus vs non-target

stimulus-evoked), layers, and frequency band, there was a significant interaction effect of layer pair and time window (three-way ANOVA, $p = 0.0075$).

Finally, we sought to compare the predictive power of our results on the monkey's perceptual performance. We created a generalized linear model (GLM) to regress behavioral outcome from the pupil diameter, number of microsaccades in the pre-target window, and average target-evoked multi-unit firing rate in each of the three layers (see Experimental Procedures; 78). Other reported measures (Fano factor, PPC, interlaminar SSC) that we could not estimate reliably on a single trial basis were not considered in the GLM analysis. Pre-target microsaccades were by far the strongest predictor of performance ($weight = -1.3116$; $p = 6.0757e-08$). Input layer firing rate also significantly predicted perception ($weight = 0.3276$; $p = 0.020068$). Superficial firing rate, deep firing rate, and pupil diameter were not significant predictors (Table 2, all $p > 0.5$). This indicates that, among the variables that we could estimate reliably on a single trial basis, stable retinal images in the pre-target window are critical for behavioral performance, and elevated firing in the input layer is the most reliable physiological signature of a perceived stimulus.

DISCUSSION

We investigated the physiological processes responsible for variable behavioral outcomes at perceptual threshold. Controlling for *both* the attentive instruction (thus minimizing large-scale attentional effects) and the stimulus condition that elicited performance at a threshold level allowed us to examine the physiological and neural correlates that underlie correct versus incorrect behavioral outcomes. While this study cannot disentangle the independent roles of behavioral state fluctuations and neural

236 fluctuations in determining behavioral outcomes, evidence suggests that differences in
237 both are associated with hits. We found multiple lines of evidence which suggest that a
238 state of higher arousal and eye-position stability and the accompanying enhanced
239 processing of visual stimuli contributes to accurate perception in hit trials (Figure 8).

240 Pupil diameter is elevated in hit trials (Figure 2A-C; Figure 8A), and prior studies
241 have shown that pupil diameter is strongly linked to arousal and alertness (51, 52, 54).
242 This provides evidence that a state of higher arousal may contribute to improved sensory
243 processing. The much lower hit rate in trials with a microsaccade preceding the target
244 (Figure 2D; Figure 8A) and our GLM analysis shows that stability of retinal images is
245 critical for accurate discrimination at threshold. It is unlikely that these two measures are
246 reflecting the same phenomenon, as there is a very weak correlation between them over
247 the course of a trial (Figure 2-figure supplement 1B).

248 There is a strong link between oculomotor control and attentional deployment (79-
249 81). In this study, hits and misses differ in their behavioral responses, with hit trials being
250 characterized by a saccade to the target stimulus. Almost all of our neural results reflect
251 differences around the time of non-target stimulus presentations during which the
252 monkeys maintained fixation at the center of the screen and, therefore, were hundreds of
253 milliseconds prior to saccade planning and execution in the case of hit trials. Trials in
254 which saccades were made to non-target stimuli were excluded from analysis, as were
255 trials in which the monkey made a saccade to the target too soon after its presentation to
256 have been a behavioral response to stimulus perception (see Methods). The analysis of
257 microsaccade occurrence focused on the window just before target stimulus presentation
258 and before monkeys could begin oculomotor planning. Only the analysis of neural

259 responses to target stimuli appears in conjunction with divergent oculomotor behavior
260 between the hit (saccade) and miss (no saccade) trials. However, here too firing rates
261 diverge much earlier, particularly in the input layer, than would be consistent with the
262 effects of saccade planning (Figure 3-figure supplement 1B; 72).

263 A body of evidence (See 82 for review), suggests that microsaccades directed
264 towards a target stimulus reflect attention-related processing and performance (65-71).
265 In our dataset, during the pre-target period, microsaccades towards the attended stimulus
266 were overrepresented in correct trials (Figure 2-figure supplement 1A, upper left).
267 Conversely, microsaccades towards the attended stimulus were underrepresented in
268 incorrect trials (Figure 2-figure supplement 1A, lower left). Microsaccades directed
269 towards the location of the eventual target may reflect elevated attentional deployment
270 that can compensate for the reduced sensitivity due to higher incidence of
271 microsaccades.

272 Our electrophysiological findings and their laminar patterns associated with hit
273 trials *within* a cued attention state mirror several previous findings that are associated
274 with the deployment of covert spatial attention. Attention has long been known to increase
275 firing rates in V4 (21, 25, 83), and there is evidence that this increase occurs in all cortical
276 layers in V4 (39). We find that elevated firing rates in hits occur across all layers in
277 conjunction with elevated arousal (Figure 3; Figure 8C). Attention reduces the variability
278 in the firing of V4 neurons, and this reduction is thought to contribute to the improved
279 information coding capacity of a population of neurons (24-26, 39, 84). The reduction in
280 Fano factor among broad-spiking superficial-layer neurons in hit trials mirrors the effects
281 of attention (Figure 4). Multiple lines of evidence suggest broad- and narrow-spiking

282 correspond to putative excitatory and inhibitory neurons respectively. Narrow-spiking
283 neurons exhibit higher firing rates, which corresponds well with inhibitory interneuron (31,
284 39, Supplementary Table 1, 40, 85-87). Repolarization times in broad-spiking neurons
285 are also longer, as they are in excitatory pyramidal neurons (40, 50, 88). Since these
286 neurons are putative projection neurons to downstream cortical areas, this reduction in
287 Fano factor may indicate increased reliability in stimulus encoding that could contribute
288 to hits. Our finding is also in agreement with previous reports of higher variability in
289 representations of unperceived stimuli in humans (89). Synchronous neural activity
290 appears to modulate perceptual and cognitive ability in a variety of contexts (90-93). We
291 found that deep-layer neurons exhibit less low-frequency phase-locking in hit trials (Figure
292 5). This is consistent with prior studies that find an attention-mediated reduction in the
293 power spectrum of the spike-triggered-averaged LFP (91).

294 Our examination of inter-laminar synchrony revealed two interesting and
295 complementary patterns: hits were associated with greater coherence between the
296 superficial and deep layers during spontaneous activity in the pre-stimulus period (Figure
297 6; Figure 8B); in contrast, we found enhanced coherence between the input layer and
298 both the output layers (superficial and deep) in the stimulus-evoked period during hits
299 (Figure 7; Figure 8C). Increased superficial-deep coherence in the pre-stimulus period
300 could be the result of neuromodulatory or top-down processes that maintain the cortex in
301 a state of sustained depolarization corresponding to a state of higher arousal during hits
302 (8, 15). Increased synchrony between the input layer and the output layers during the
303 stimulus-evoked period could then reflect stronger information propagation through the
304 cortical circuit, and hence with improved stimulus detection (94). In contrast to broad

305 global synchrony or local correlated fluctuations, which may signal a default state of
306 minimal processing or decreased information coding capacity (26, 95-97), these patterns
307 of interlaminar coherence that we found suggest that successful perception at threshold
308 is mediated by pathway specific modulation of information flow through the laminar
309 cortical circuit.

310 Taken together, our results provide insight about how information about a
311 threshold stimulus may successfully propagate through a cortical column and influence
312 sensory perception. Lower baseline variability among broad-spiking superficial layer
313 neurons and decreased low-frequency synchronous activity in the deep layers could be
314 indicative of improved capacity to encode sensory information. Higher target-evoked firing
315 rates and elevated interlaminar synchrony could enhance the propagation of this encoded
316 signal. These results associate pre-stimulus baseline state differences with enhanced
317 cortical processing in the stimulus-evoked period.

318 Several studies have examined how information flow differs for perceived and
319 unperceived stimuli at a more macroscopic scale (4, 9). van Vugt et al. (9) recorded from
320 three brain regions, V1, V4, and dorsolateral prefrontal cortex (dlPFC), while a monkey
321 performed a stimulus detection task at threshold. Their work supports the model that
322 feedforward propagation of sensory information from the visual cortex to the PFC causes
323 a non-linear “ignition” of association areas resulting in conscious perception (98). Herman
324 et al. (4) found that conscious human perception triggers a wave of activity propagation
325 from occipital to frontal cortex while switching off default mode and other networks. Our
326 study provides insight into the functions of the cortical microcircuit at the columnar level
327 that could reflect these large-scale sweeping activity changes in perception.

328 Overall, we identified substantial layer-specific differences in cortical activity
329 between hits and misses at perceptual threshold, leading to the following conceptual
330 model (Figure 8). During spontaneous activity, the state of elevated arousal and eye
331 position stability during hits (Figure 8A) is manifested by increased interlaminar synchrony
332 between the superficial and deep layers (Figure 8B, thicker orange arrows), which we
333 propose is due to top-down influences. We predict that decreased firing variability in
334 broad-spiking neurons in the superficial layer is caused by a lower variability in membrane
335 potential closer to the action potential threshold among these neurons (Figure 8B, inset).
336 Elevated feed-forward propagation in the stimulus-evoked period (Figure 8C) and a
337 membrane potential closer to action potential threshold could both contribute to higher
338 firing rates in the output layers of the cortex (Figure 8C, inset), and are indicative of
339 greater fidelity of stimulus processing in hits. These physiological differences in the
340 laminar microcircuit likely contribute to successful perceptual discrimination at threshold.

341 **MATERIALS & METHODS**

342 **Surgical Procedures**

343 Surgical procedures have been described in detail previously (39, 99, 100). In brief, an
344 MRI compatible low-profile titanium chamber was placed over the pre-lunate gyrus, on
345 the basis of preoperative MRI in two rhesus macaques (right hemisphere in Monkey A,
346 left hemisphere in Monkey C). The native dura mater was then removed, and a silicone
347 based optically clear artificial dura (AD) was inserted, resulting in an optical window over
348 dorsal V4 (Figure 1-figure supplement 1A, B). Antibiotic (amikacin or gentamicin) soaked
349 gauzed was placed in the chamber between recording sessions to prevent bacterial

350 growth. All procedures were approved by the Institutional Animal Care and Use
351 Committee and conformed to NIH guidelines.
352
353 **Electrophysiology**
354 At the beginning of each recording session a plastic insert, with an opening for targeting
355 electrodes, was lowered into the chamber and secured. This served to stabilize the
356 recording site against cardiac pulsations. Neurons were recorded from cortical columns
357 in dorsal V4 using 16-channel linear array electrodes ('laminar probes', Plexon Inc.,
358 Plexon V-probe). The laminar probes were mounted on adjustable X-Y stages attached
359 to the recording chamber and positioned over the center of the pre-lunate gyrus under
360 visual guidance through a microscope (Zeiss Inc., Figure 1-figure supplement 1C). This
361 ensured that the probes were maximally perpendicular to the surface of the cortex and
362 thus had the best possible trajectory to make a perpendicular penetration down a cortical
363 column. Across recording sessions, the probes were positioned over different sites along
364 the center of the gyrus in the parafoveal region of V4 with receptive field (RF)
365 eccentricities between 2 and 7 degrees of visual angle. Care was taken to target cortical
366 sites with no surface micro-vasculature, with surface micro-vasculature used as reference
367 so that the same cortical site was not targeted across recording sessions. The probes
368 were advanced using a hydraulic microdrive (Narishige Inc.) to first penetrate the AD and
369 then through the cortex under microscopic visual guidance. Probes were advanced until
370 the point that the top-most electrode (toward the pial surface) registered local field
371 potential (LFP) signals. At this point, the probe was retracted by about 100-200 μm to
372 ease the dimpling of the cortex due to the penetration. This procedure greatly increased

373 the stability of the recordings and increased the neuronal yield in the superficial
374 electrodes.

375 The distance from the tip of the probes to the first electrode contact was either 300
376 μm or 700 μm. The inter-electrode distance was 150 μm, thus minimizing the possibility
377 of recording the same neural spikes in adjacent recording channels. Electrical signals
378 were recorded extracellularly from each channel. These were then amplified, digitized
379 and filtered either between 0.5 Hz and 2.2 kHz (LFPs) or between 250 Hz and 8 kHz
380 (spikes) and stored using the Multichannel Acquisition Processor system (MAP system,
381 Plexon Inc.). Spikes and LFPs were sampled at 40 and 10 kHz respectively. LFP signals
382 were further low-pass filtered with a 6th order Butterworth filter with 300Hz cut-off and
383 down-sampled to 1 kHz for further analysis. Spikes were classified as either multi-unit
384 clusters or isolated single units using the Plexon Offline Sorter software program. Single
385 units were identified based on two criteria: (a) if they formed an identifiable cluster,
386 separate from noise and other units, when projected into the principal components of
387 waveforms recorded on that electrode and (b) if the inter-spike interval (ISI) distribution
388 had a well-defined refractory period. Single-units were classified as either narrow-spiking
389 (putative interneurons) or broad-spiking (putative pyramidal cells) based on methods
390 described in detail previously (25, 39). Specifically, only units with waveforms having a
391 clearly defined peak *preceded* by a trough were potential candidates. The distribution of
392 trough-to-peak duration was clearly bimodal (Hartigan's Dip Test, $p = 0.012$) (101). Units
393 with trough-to-peak duration less than 225 μs were classified as narrow-spiking units;
394 units with trough-to-peak duration greater than 225 μs were classified as broad-spiking
395 units (Figure 1-figure supplement 1D; teal=narrow, gold=broad).

396 Data was collected over 32 sessions (23 sessions in Monkey A, 9 in Monkey C),
397 yielding a total of 413 single units (146 narrow-spiking, 267 broad-spiking) and 296 multi-
398 unit clusters. Per session unit yield was considerably higher in Monkey C compared to
399 Monkey A, resulting in a roughly equal contribution of both monkeys toward the population
400 data.
401
402 **Task, Stimuli and Inclusion Criteria**
403 Stimuli were presented on a computer monitor placed 57 cm from the eye. Eye position
404 was continuously monitored with an infrared eye tracking system (ISCAN ETL-200). Trials
405 were aborted if eye position deviated more than 1° (degree of visual angle, 'dva') from
406 fixation. Experimental control was handled by NIMH Cortex software
407 (http://www.cortex.salk.edu/). Eye-position (all sessions) and pupil diameter (18/32
408 sessions) data were concurrently recorded and stored using the MAP system.
409 *Receptive Field Mapping*: At the beginning of each recording session, neuronal
410 RFs were mapped using subspace reverse correlation in which Gabor (eight orientations,
411 80% luminance contrast, spatial frequency 1.2 cycles/degree, Gaussian half-width 2°) or
412 ring stimuli (80% luminance contrast) appeared at 60 Hz while the monkeys maintained
413 fixation. Each stimulus appeared at a random location selected from an 11x11 grid with
414 1° spacing in the appropriate visual quadrant. Spatial receptive maps were obtained by
415 applying reverse correlation to the evoked local field potential (LFP) signal at each
416 recording site. For each spatial location in the 11x11 grid, we calculated the time-
417 averaged power in the stimulus evoked LFP (0-200ms after each stimulus flash) at each
418 recording site. The resulting spatial map of LFP power was taken as the spatial RF at the

recording site. For the purpose of visualization, the spatial RF maps were smoothed using spline interpolation and displayed as stacked contours plots of the smoothed maps (Figure 1-figure supplement 1G). All RFs were in the lower visual quadrant (lower-left in Monkey A, lower-right in Monkey C) and with eccentricities between 2 and 7 dva.

Current Source Density Mapping: In order to estimate the laminar identity of each recording channel, we used a current source-density (CSD) mapping procedure (48). Monkeys maintained fixation while 100% luminance contrast ring stimuli were flashed (30ms) centered at the estimated RF overlap region across all channels. The size of the ring was scaled to about three-quarters of the estimated diameter of the RF. CSD was calculated as the second spatial derivative of the flash-triggered LFPs (Figure 1-figure supplement 1E). The resulting time-varying traces of current across the cortical layers can be visualized as CSD maps (Figure 1-figure supplement 1F; maps have been spatially smoothed with a Gaussian kernel for aid in visualization). Red regions depict current sinks in the corresponding region of the cortical laminae; blue regions depict current sources. The input layer (Layer 4) was identified as the first current sink followed by a reversal to current source. The superficial (Layers 1-3) and deep (Layers 5-6) layers had opposite sink-source patterns. LFPs and spikes from the corresponding recording channels were then assigned to one of three layers: superficial, input or deep.

Attention task: In the main experiment, monkeys had to perform an attention-demanding orientation change-detection task (Figure 1A). While the monkey maintained fixation, two achromatic Gabor stimuli (orientation optimized per recording session, spatial frequency 1.2 cycles/degree, 6 contrasts randomly chosen from an uniform distribution of luminance contrasts, $c = [10, 18, 26, 34, 42, 50\%]$) were flashed on for 200

ms and off for a variable period chosen from a uniform distribution between 200-400 ms. One of the Gabors was flashed at the receptive field overlap region, the other at a location of equal eccentricity across the vertical meridian. At the beginning of a block of trials, the monkey was spatially cued ('instruction trials') to covertly attend to one of these two spatial locations. During these instruction trials, the stimuli were only flashed at the spatially cued location. No further spatial cue was presented during the rest of the trials in a block. At an unpredictable time drawn from a truncated exponential distribution (minimum 1 s, maximum 5 s, mean 3 s), one of the two stimuli changed in orientation. The monkey was rewarded for making a saccade to the location of orientation change. The monkey was rewarded for only those saccades where the saccade onset time was within a window of 100-400 ms after the onset of the orientation change. The orientation change occurred at the cued location with 95% probability and at the uncued location with 5% probability ('foil trials'). We controlled task difficulty by varying the degree of orientation change (Δ_{ori}), which was randomly chosen from one of the following: 1, 2, 3, 4, 6, 8, 10 and 12°. The orientation change in the foil trials was fixed at 4°. These foil trials allowed us to assess the extent to which the monkey was using the spatial cue, with the expectation that there would be an impairment in performance and slower reaction times compared to the case in which the change occurred at the cued location. If no change occurred before 5s, the monkey was rewarded for maintaining fixation ('catch trials', 13% of trials). We refer to all stimuli at the baseline orientation as 'non-targets' and the stimulus flash with the orientation change as the 'target'.

Inclusion criteria: Of the 413 single units, we included only a subset of neurons that were visually responsive for further analysis. For each neuron we calculated its

465 baseline firing-rate for each attention condition (attend into RF [‘attend-in’ or ‘IN’], attend
466 away from RF [‘attend-away’ or ‘AWAY’]) from a 200ms window before a stimulus flash.
467 We also calculated the neuron’s contrast response function for both attention conditions
468 (Figure 1-figure supplement 1H). This was calculated as the firing rate over a window
469 between 60-200 ms after stimulus onset and averaged across all stimulus flashes
470 (restricted to non-targets) of a particular contrast separately for each attention condition.
471 A neuron was considered visually responsive if any part of the contrast response curves
472 exceeded the baseline rate by 4 standard deviations for both attention conditions. This
473 left us with 274 single units (84 narrow-spiking, 190 broad-spiking) and 217 multi-unit
474 clusters for further analysis.
475
476 **Data analysis**
477 *Behavioral Analysis*: For each orientation change condition Δ_{ori}, we calculated the
478 hit rate as the ratio of the number of trials in which the monkey correctly identified the
479 target by making a saccadic eye-movement to the location of the target over the number
480 of trials in which the target was presented. The hit rate as a function of Δ_{ori}, yields a
481 behavioral psychometric function (Figure 1B). We performed this analysis independently
482 for each recording day for each monkey, yielding a similar but distinct psychometric
483 function for every session. Psychometric functions were fitted with a smooth logistic
484 function (1). Error bars were obtained by a jackknife procedure (20 jackknives, 5% of trials
485 left out for each jackknife). Performance for the foil trials were calculated similarly as the
486 hit rate for trials in which the orientation change occurred at the un-cued location (Figure
487 1B, square symbol). For each fitted psychometric function in both the attend-in and

488 attend-away conditions, we calculated the threshold of the fitted logistic function (i.e. the
489 Δ_{ori} at which performance was mid-way between the lower and upper asymptotes).
490 Because the threshold of the fitted function always lies somewhere on the axis of Δ_{ori}, but
491 not exactly at an orientation change presented to the subject, we then defined the
492 threshold condition as the subset of trials in which the orientation change of the target
493 stimulus was closest to the threshold of the fitted function (Figure 1B). We restricted
494 further analysis to this threshold condition. For this threshold condition we identified the
495 trials in which the monkey correctly identified the target as 'hit' trials and those in which
496 the monkey failed to identify the target as 'miss' trials. Analysis of behavior, pupil
497 diameter, and microsaccades was conducted on both the attend-in and attend-away
498 conditions; all electrophysiological analysis was applied only to the attend-in condition.

499 *Pupil Diameter*: The raw pupil diameter measurements from the infrared eye-
500 tracking system could differ across days due to external factors such as display monitor
501 illumination. To control for this, we normalized the raw data by a Z-score procedure
502 separately for each session (using the mean and standard deviation of all measurements
503 during the session). We analyzed normalized pupil diameter traces for hit and miss trials
504 in the threshold condition, over a time window from 100 ms before to 100 ms after all
505 stimulus presentations (non-target and target), excluding the first stimulus presentation in
506 a trial. The first stimulus was excluded to avoid pupil diameter changes due to the pupillary
507 near response caused by acquiring fixation (102). The pupil diameter was averaged over
508 this time period and compared across conditions using bootstrap estimation and *t*-test.
509 Distribution violin plots were generated using kernel density estimation (103)
510 (bandwidth(hit) = 0.0801, bandwidth(miss) = 0.0648).

511 *Microsaccade Analysis:* Saccadic eye-movements were detected using ClusterFix
512 (104). We identified microsaccades by filtering for eye movements with amplitudes
513 between 0.1 and 1 degree of visual angle. We then split all trials in the threshold condition
514 into two groups: those in which a microsaccade was detected in the 400ms preceding the
515 target stimulus presentation, and those without a detected microsaccade. We calculated
516 the hit rate for trials within those two groups. For all trials in which a target stimulus was
517 presented at the attended location, we determined the direction of all microsaccades in
518 the 400ms period preceding target presentation, relative to both the attended and
519 unattended stimuli. The relative microsaccade direction was defined as the angle
520 between two vectors: the one defined by the eye positions at the beginning and end of
521 the microsaccade, and the vector from the initial eye position to the center of the stimulus
522 (calculated separately for attended and unattended stimuli). Relative microsaccade
523 directions were grouped into 12 bins from 0-360°. The distribution of relative
524 microsaccade directions were calculated separately for correct and incorrect trials,
525 relative to both the attended and unattended stimuli (Figure 2-figure supplement 1A).
526 We next created a null distribution of relative microsaccade direction. This was
527 done by pooling together microsaccades from correct and incorrect trials and then
528 sampling with replacement from this pooled data (bootstrap procedure (105); 1000
529 samples). The number of microsaccades chosen for each sample was the same as the
530 number in correct or incorrect trials respectively. These bootstrapped samples were used
531 to create 99.5% confidence intervals for the count of microsaccades expected in each of
532 the 12 bins. A bin was considered significantly different from chance if it's true count fell
533 outside this confidence interval.

534 We calculated microsaccade rate for an entire trial by dividing the total number of
535 detected microsaccades in the whole trial by the trial length (4592 total trials). The
536 Pearson correlation between microsaccade rate and mean normalized pupil diameter
537 (see above) for the trial was calculated for all trials with pupil diameter data, regardless
538 of trial type or outcome (Figure 2-figure supplement 1B). Not pictured in Figure 2-figure
539 supplement 1B but included in correlation analysis were trials with a mean normalized
540 pupil diameter greater than 2 or less than -2 (~4% of trials). Only 4 of these trials were
541 longer than 1 s, out of which 2 trials contained detected microsaccades. The mean pupil
542 diameter in these trials is shown in Figure 2-figure supplement 1B inset. Inter-
543 microsaccade time was calculated as the time between microsaccade onset of
544 microsaccades detected in the same trial. 4% of microsaccades separated by >538 ms
545 are excluded from Figure 2-figure supplement 1D as they were more than 1.5x the
546 interquartile range above the third quartile.

547 *Firing Rate:* Firing rates were normalized per neuron to that neuron's maximum
548 stimulus-evoked response to each contrast before being combined across contrasts and
549 trial types. We averaged stimulus-evoked firing rates from 60-260 ms following non-target
550 or target stimulus presentations. We used bootstrapped estimation to compare firing rates
551 in hit and miss trials in a paired comparison. This was done for all single and multi-unit
552 clusters, as well as broad- and narrow-spiking single-units in each layer. Firing rates were
553 also compared across hit and miss trials by paired *t*-test for each group. PSTH of firing
554 rates were calculated in 30ms bins shifted in 5ms increments. To calculate the time of
555 firing rate divergence, we compared the difference in each single neuron or multi-unit
556 firing rate in the two conditions over time. At each time point, we performed a Wilcoxin

rank-sum test comparing the firing rates across hits and misses, and defined the divergence point as the first time the firing rates were significantly different. Divergence was calculated separately for each layer. To determine the time at which firing rates rose above baseline levels, we used bootstrapping to estimate 95% confidence intervals for each neuron's pre-stimulus firing rate (0-100 ms before target or non-target stimulus onset). We then calculated the target PSTH for each neuron in 30ms bins shifted in 5ms increments. We defined the response latency as the first time bin in which the neuron's firing rate in the PSTH exceeded the upper limit of the 95% confidence interval of baseline firing. We calculated the response latency independently for hit and miss trials for each neuron.

Fano factor: Trial-to-trial variability was estimated by the Fano factor, which is the ratio of the variance of the spike counts across trials over the mean of the spike counts for each broad and narrow-spiking single unit. The Fano factor was calculated over non-overlapping 20ms time bins in a window from 200ms prior to each non-target flash onset to 200ms after each non-target flash onset for hit and miss trials in the threshold condition. To compare across conditions, we calculated the Fano factor modulation index (MI), defined as

$$\mathrm{MI} = \frac{FF_{hit} - FF_{miss}}{FF_{hit} + FF_{miss}}$$

where FF_{hit} and FF_{miss} represent the Fano factor for a given unit in hit and miss trials respectively at each point in time with respect to non-target stimulus onset. The Fano factor MI was averaged from 0-60ms prior to non-target stimulus onset and compared across trial types in the threshold condition for each sub-population.

Pairwise Phase Consistency (PPC): We calculated PPC (76) for single and multi-units in the non-target pre-stimulus period (0-200ms preceding onset) in trials in the threshold condition. Although PPC is unbiased by spike count, we set a threshold of 50 spikes for analysis so that only units with enough spikes for a reliable estimate of PPC were included (superficial: $n = 26$, input: $n = 41$, deep: $n = 64$). LFP phase was calculated using Morlet wavelets. PPC for each unit was calculated for the phase of the LFP recorded on the same channel and averaged in three frequency bands (3-12 Hz, 15-25 Hz, and 30-80 Hz). PPC was calculated separately for hit and miss trials and compared across trial outcomes by t-test, corrected for multiple comparisons.

Spike-spike coherence (SSC): For each recording session, all spikes recorded from visually responsive single and multi-units in each layer were combined into a single spike train for that layer (layer multi-unit). Separately for both the pre-stimulus and non-target stimulus-evoked periods, we randomly deleted spikes from the layer multi-unit with a higher firing rate so that the firing rates were matched across hit and miss trials. SSC was calculated for each of the three possible pairs of layer multi-units in each session for both the pre-stimulus (0-200 ms preceding stimulus onset) and non-target stimulus evoked period (60-260 ms following non-target stimulus onset) separately for hit and miss trials using Chronux (NW = 1; K = 1; http://chronux.org) (77, 106). To control for differences in firing rates across hit and miss trials we used a rate matching procedure (26). For estimation statistics, interlaminar SSC values was calculated for each frequency and subsequently averaged across three frequency bands: 3-12 Hz, 5-15 Hz, and 30-80 Hz and compared across hit and miss trials for each pair of layers in each recording session. For null-hypothesis testing, we calculated the SSC modulation index, defined as

$$\mathrm{MI} = \frac{SSC_{hit} - SSC_{miss}}{SSC_{hit} + SSC_{miss}}$$

The SSC MI was calculated for each frequency and subsequently averaged across three frequency bands: 3-12 Hz, 5-15 Hz, and 30-80 Hz. MI values for each frequency band were compared to zero by t-test, Bonferroni corrected for multiple comparisons. We tested for interaction effects with a three-factor ANOVA, with frequency, pair of layers, and time window (pre or post stimulus) as factors. We calculated a shuffled distribution of SSC by shuffling the trial identities of the spikes in one of the layers in the pair. We then calculated SSC with the shuffled trial identities. This procedure was repeated 10 times to create the shuffled distribution.

GLM quantification: To compare how well our results can predict behavioral performance we fit a GLM to the response of the monkeys in trials in the threshold condition (78). We included five regressors in our analysis: (1) average pupil diameter during the trial, (2) number of microsaccades in the pre-target window (0-400ms before target stimulus onset), and average target-evoked multi-unit firing rate in the (3) superficial, (4) input, and (5) deep layers. We calculated the average target-evoked firing rate by averaging the firing rate of all single- and multi-units in a given layer 60-260ms after target stimulus onset in each trial. In order to be able to compare weights across regressors, each regressor was transformed into a z-score before being included in the model. We fit the GLM using a logit link function, using the predictors to regress the categorical binary trial outcome (hit or miss). A total of 309 trials were included in the GLM.

FIGURE LEGENDS

Figure 1. Orientation change detection task at perceptual threshold

(**A**) Schematic of task structure. The monkey initiated a trial by fixating on the center of the screen. Two Gabor stimuli (represented by oriented lines) were presented for 200 ms and then turned off for 200-400ms. This was repeated until, at an unpredictable time, one of the stimuli changed orientation. The monkey could report having seen the change by making an eye movement to the location of the target stimulus to receive a reward (hit trials). If the monkey failed to report the orientation change and maintained fixation on the center of the screen it was not rewarded (miss trials). Before a block of trials, the monkey was cued as to which stimulus was likely to undergo the change (95% valid cue). In 5% of trials the orientation change occurred at the other location (foil trials). Circles indicating the cued location and receptive field are drawn for figure reference only and were not presented during the task. (**B**) Example behavioral psychometric function from one recording session and attention condition. Behavioral performance (hit rate, circles) is presented as a function of orientation change. Data was fitted with a logistic function. The threshold condition, trials with performance halfway between the upper and lower asymptotes of the logistic function, is indicated by the orange box. Error bars represent standard deviation calculated with a jackknife procedure (20 jackknives). The square symbol indicates foil trial performance.

Figure 2. Hit trials have larger pupil diameter whereas microsaccades more often precede misses

(**A**) Normalized pupil diameter for hit and miss trails in the threshold condition. 0 ms corresponds to non-target and target stimulus onset. Mean +/- s.e.m. (**B**) Distribution of pupil diameter values associated with hit and miss trials. Pupil diameter was averaged from 100ms before to 100ms after non-target and target stimulus onset. Violin plots were generated using kernel smoothing (See Experimental Procedures). Error bars represent 95% confidence intervals for the mean of each distribution, and the mean difference (blue, right axes). *Inset*: zoomed in view of the mean difference between hit and miss trials. Black bar represents a 95% confidence interval of the mean difference. Shaded region reflects the distribution of the bootstrapped estimation of the mean difference. (**C**) Histogram of mean pupil diameter around the time of non-target and target stimulus onset (calculated as in **B**). Orange and gray lines represent the mean pupil diameter for hit and miss trials respectively. (**D**) *Left:* Hit rate for trials with (387 trials) and without (*right*, 1336 trials) a microsaccade detected in the time window 0-400ms before target onset. *Right:* Bootstrapped estimation of the mean difference in hit proportion in trials with vs without a pre-target microsaccade. Same conventions as **2B**.

Figure 3. Target stimuli evoke higher firing rates in hit trials

Rows correspond to different layers (top=superficial, middle=input, bottom=deep). (**A**) Population (visually responsive single and multi-unit) PSTH for non-target stimuli during hit (orange) and miss (dark-gray) trials in the threshold condition (mean +/- s.e.m). The horizontal black bar indicates the time and duration of stimulus presentation. (**B**) As in **A** but for target stimuli. The star indicates the time at which firing rates in the input layer first differ significantly between hit and miss trials. Vertical lines represent the mean time firing rates for each neuron rise above the 95% confidence interval of their baseline activity (see also Figure 3-figure supplement 1C). (**C**) Bootstrapped estimation of the paired mean difference in target stimulus-evoked firing rate across hit and miss trials in the time window 60-260ms (red dotted box in **B**) after target stimulus onset. Shaded regions represent the bootstrapped estimation of the paired mean difference in firing rate (hit - miss), and black lines are 95% confidence intervals. Plots include data from both single and multi-units, separated by layer (top=superficial, middle=input, bottom=deep). (**D**) As in **C**, bootstrapped estimation of the paired mean difference in firing rate for hit trials compared to miss trials in the target stimulus-evoked period, but only for single-units broken up by cell class (gold=broad, teal=narrow).

Figure 4. Broad-spiking neurons in the superficial layer have decreased variability in hit trials

(**A**) Rows correspond to different layers (top=superficial, middle=input, bottom=deep). The Fano factor of broad-spiking putative excitatory neurons for the hit and miss trials in the threshold condition (mean +/- s.e.m). There is a significant decrease in variability for the hit trials prior to stimulus onset only in the superficial layer. 0 ms corresponds to non-target stimulus onset. The average Fano factor within a 60ms time-window (red dashed box) prior to non-target stimulus onset is plotted in **B**. (**B**) *Top:* Fano factor modulation index for each broad-spiking neurons recorded in each layer, averaged in the 60ms preceding non-target stimulus onset. *Bottom:* Bootstrapped estimation of the mean difference of the Fano factor

modulation index from zero in each of the three layers. Colored curves represent the estimated bootstrapped distribution. Black dots and lines reflect the mean and 95% confidence intervals of the distributions.

Figure 5. Deep layer neurons are phase-locked to low-frequency rhythms in miss trials
(**A**) Pairwise phase consistency (PPC) of single and multi-units in each layer to the local field potential (LFP) signal recorded from the same channel in hit and miss trials at threshold. PPC was calculated in the pre-stimulus period (0-200 ms before stimulus onset). Dashed red line indicates a PPC of 0, below which there is no consistent relationship between spikes and LFP phase. (**B**) Bootstrapped estimation plot for the paired mean difference in PPC for deep layer neurons over three frequency bands: 3-12Hz, 15-25Hz, 30-80Hz. Curves represent the bootstrapped distribution for the paired difference, and black dots and vertical lines represent the mean and 95% confidence intervals for the paired mean difference

Figure 6. Greater interlaminar coherence in hit trials in the pre-stimulus period
Interlaminar spike-spike coherence in the pre-stimulus period (0-200ms prior to stimulus onset). Rows correspond to different pairs of layers (*top*=superficial-input, *middle*=superficial-deep, *bottom*=input-deep). (**A**) Multi-unit interlaminar spike-spike coherence (SSC) calculated in the 200ms before non-target stimulus onset in hit and miss trials (solid lines, mean +/- s.e.m). Firing rates were matched across hit and miss trials. Dashed lines represent coherence calculated with shuffled trial identities (mean +/- s.e.m). (**B**) Bootstrapped estimation plot for the paired mean difference in SSC for each pair of layers averaged over three frequency bands : 3-12Hz, 15-25Hz, 30-80Hz. Curves represent the bootstrapped distribution for the paired difference, and black dots and vertical lines represent the mean and 95% confidence intervals for the paired mean difference.

Figure 7. Greater interlaminar coherence in hit trials in the stimulus-evoked period
Interlaminar spike-spike coherence in the stimulus evoked period (60-260ms after stimulus onset). Same conventions as in Figure 6.

Figure 8. Conceptual model for stimulus processing at perceptual threshold
(**A**) Hit trials have a larger pupil diameter and fewer pre-target microsaccades, reflecting a state of increased arousal and greater eye position stability. Conversely, miss trials show decreased arousal and eye position stability. (**B**) In the spontaneous pre-stimulus period, hits are characterized by decreased variability in superficial layer broad-spiking neurons, which we hypothesize is reflective of lower membrane potential (V_m) variability (inset). Hit trials are also characterized by greater synchrony between the superficial and deep layers (indicated by thicker arrows), which could be reflecting a stronger top-down influence on the cortical column. (**C**) In the stimulus-evoked period there is greater interlaminar synchrony between pairs that include the input layer (represented by thicker arrows), which we propose reflects improved feed-forward propagation of information. We propose these state differences in hits contribute to elevated firing rates in response to target stimuli, particularly in the superficial layers (inset), resulting in a higher-fidelity output to downstream areas. E = excitatory; I = inhibitory; s = superficial; i = input; d = deep.

Figure 1-figure supplement 1. Laminar recordings in V4
(**A**) An artificial dura (AD) chamber is shown over dorsal V4 in the right hemisphere of Monkey A. The native dura mater was resected and replaced with a silicone based artificial dura, thereby providing an optically clear window into the cortex. Scale bar = 5mm. (**B**) An enlarged view of the boxed region in **A** clearly shows the sulci and the microvasculature. sts = superior temporal sulcus, lu = lunate sulcus, io = inferior occipital sulcus. Area V4 lies on the pre-lunate gyrus between the superior temporal and lunate sulci. Scale bar = 2mm. (**C**) Electrophysiology setup: a plastic stabilizer with a circular aperture is secured in place inside the chamber such that the aperture is centered over the pre-lunate gryus. A 16-channel linear array electrode (electrode spacing 150 μm) is positioned over the center of the gyrus and lowered into the cortex under microscopic guidance. The microvasculature pattern was used as a reference to target different cortical sites across recording sessions. (**D**) Example recording session in monkey C depicting 12 single unit waveforms (mean +/- s.e.m.) isolated along the cortical column. Teal waveforms correspond to narrow-spiking putative interneurons and gold waveforms correspond to broad-spiking putative excitatory units. (**E**) Stimulus triggered local field potentials (LFPs) obtained by flashing 30ms high contrast ring stimuli in the receptive field of a V4 cortical column. LFP traces averaged across all stimulus repeats are shown color-

coded as being part of either the superficial (green), input (gray) or deep (pink) layers. Layer assignment was done after current source-density analysis. (**F**) Current source-density (CSD) calculated as the second spatial derivative of the stimulus triggered LFPs and displayed as a colored map. The x-axis represents time from stimulus onset; the y-axis represents cortical depth oriented such that the pial surface is at the top and the white matter is at the bottom. Red hues represent current sink, blue hues represent current source. The input layer is identified as the first current sink followed by a reversal to current source. The superficial and deep layers have the opposite sink-source pattern. The CSD map has been spatially smoothed for visualization. (**G**) Stacked contour plots show spatial receptive fields (RFs) mapped along each contact point in the laminar probe. The spatial receptive fields were obtained by applying reverse correlation to the LFP power evoked by sparse pseudo-random sequences of Gabor stimuli. The RFs are well aligned, indicating perpendicular penetration down a cortical column. Zero depth represents the center of the input layer as estimated from the CSD. (**H**) Contrast response functions – spikes rate as a function of stimulus contrast – are shown for 2 example units identified in a single recording session in Monkey A. Red and blue traces correspond to the attend-in to RF and attend-away from RF conditions respectively. The dotted lines represent the corresponding background firing-rates. The dashed lines are 4 standard deviations above baseline. A unit was considered as visually responsive, if the contrast response functions exceeded this threshold in both the attention conditions. Mean +/- s.e.m. Panels are reproduced from Nandy et al. (2017).

Figure 2-figure supplement 1. Microsaccades are preferentially directed towards the target in correct trials and have a slight correlation with pupil diameter

Data is presented for all trials, regardless of orientation change (not just the threshold condition). (**A**) The histograms represent the direction of microsaccades relative to the attended stimulus (left column) or unattended stimulus (right column) in correct (top row) and incorrect (bottom row) trials. Black lines represent the mean (solid) and 99.5% confidence interval (dashed) of the bootstrapped null distribution estimated by pooling correct and incorrect microsaccades. $* \mathrm{p} < 0.005$. *Inset:* Schematic for calculation of relative microsaccade direction. Microsaccade is represented by the gray arrow (**B**) Scatterplot of microsaccade rate versus mean normalized pupil diameter, shows a small but statistically significant relationship between the two quantities ($r^2 = 0.006$, $p < 0.001$). Each dot is color-coded by trial length. *Inset:* Histogram of mean pupil diameter for all trials, including those less than -2 or greater than 2 (red lines). Only four of the trials with pupil diameters less than -2 or greater than 2 had detected microsaccades. (**C**) Boxplot of microsaccade rates for all trials. (**D**) Boxplot of the time between microsaccades recorded in the same trial. 4% of microsaccades separated by more than 538ms were excluded as outliers (See Methods).

Figure 3-figure supplement 1. Firing rates for individual neurons and reaction time in threshold condition

(**A**) Target stimulus-evoked normalized firing rates in hit and miss trials for each recorded single and multi-unit cluster in hit and miss trials. Clusters are divided by layer: left=superficial, middle=input, right=deep. Related to Figure 3B. Each line represents the mean firing rate in response to target stimuli in hit and miss trials for a given unit. Data is color coded by unit type (gold=broad, teal=narrow, gray=multi-unit). See Experimental Procedures for normalization method. (**B**) Mean reaction time (time from target stimulus onset to saccade onset) for hit trials in the threshold condition in both attend-in (red) and attend-away (blue) trials for each recording session. (**C**) Mean time at which single- and multi-unit firing rates rise significantly above pre-stimulus baseline in response to target stimuli in hit and miss trials. Mean +/- s.e.m.

Figure 4-figure supplement 1. Narrow-spiking neurons do not have decreased variability in hit trials

Top: Fano factor modulation index for each narrow-spiking neurons recorded in each layer, averaged in the 60ms preceding non-target stimulus onset. *Bottom:* Bootstrapped estimation of the mean difference of the Fano factor modulation index from zero in each of the three layers. Colored curves represent the estimated bootstrapped distribution. Black dots and lines reflect the mean and 95% confidence intervals of the distributions.

Figure 5-figure supplement 1. Additional PPC data

(**A-B**) *Top:* Raw PPC values calculated for clusters recorded in the superficial (**A**) and (**B**) input layers in hit and miss trials, averaged into three frequency bands, 3-12 Hz, 15-25 Hz, and 30-80 Hz. PPC was calculated using the LFP recorded on the same channel as the spikes. *Bottom:* Bootstrapped estimation of the paired

mean difference in PPC across hit and miss trials for each frequency band. Note that although there appears to be a difference in high-frequency PPC in the superficial layer, this population does not have significantly positive PPC in either condition, indicating that there is no phase-locking in either hits or misses. (**C**) Raw PPC values for neurons recorded in the deep layer in hit and miss trials, averaged into the same 3 frequency bands. Related to Figure 5B.

AUTHOR CONTRIBUTIONS

MPJ and ASN conceptualized the project. ASN collected the data and supervised the project. MPM analyzed the data, with assistance from SD and IB. MPM, SD, ASN, MPJ, and JHR wrote the manuscript.

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Figure 1

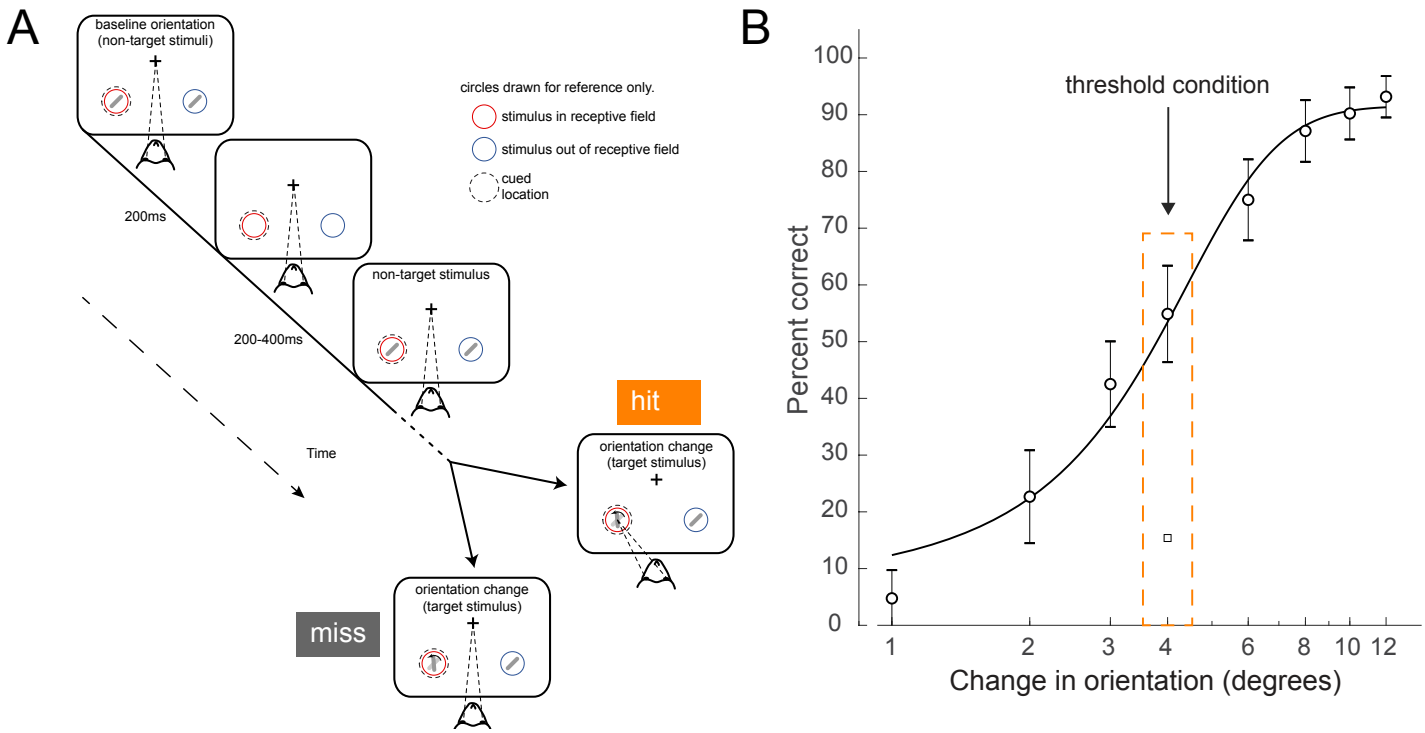

Figure 1. Orientation change detection task at perceptual threshold
(**A**) Schematic of task structure. The monkey initiated a trial by fixating on the center of the screen. Two Gabor stimuli (represented by oriented lines) were presented for 200 ms and then turned off for 200-400ms. This was repeated until, at an unpredictable time, one of the stimuli changed orientation. The monkey could report having seen the change by making an eye movement to the location of the target stimulus to receive a reward (hit trials). If the monkey failed to report the orientation change and maintained fixation on the center of the screen it was not rewarded (miss trials). Before a block of trials, the monkey was cued as to which stimulus was likely to undergo the change (95% valid cue). In 5% of trials the orientation change occurred at the other location (foil trials). Circles indicating the cued location and receptive field are drawn for figure reference only and were not presented during the task. (**B**) Example behavioral psychometric function from one recording session and attention condition. Behavioral performance (hit rate, circles) is presented as a function of orientation change. Data was fitted with a logistic function. The threshold condition, trials with performance halfway between the upper and lower asymptotes of the logistic function, is indicated by the orange box. Error bars represent standard deviation calculated with a jackknife procedure (20 jackknives). The square symbol indicates foil trial performance.

Figure 2

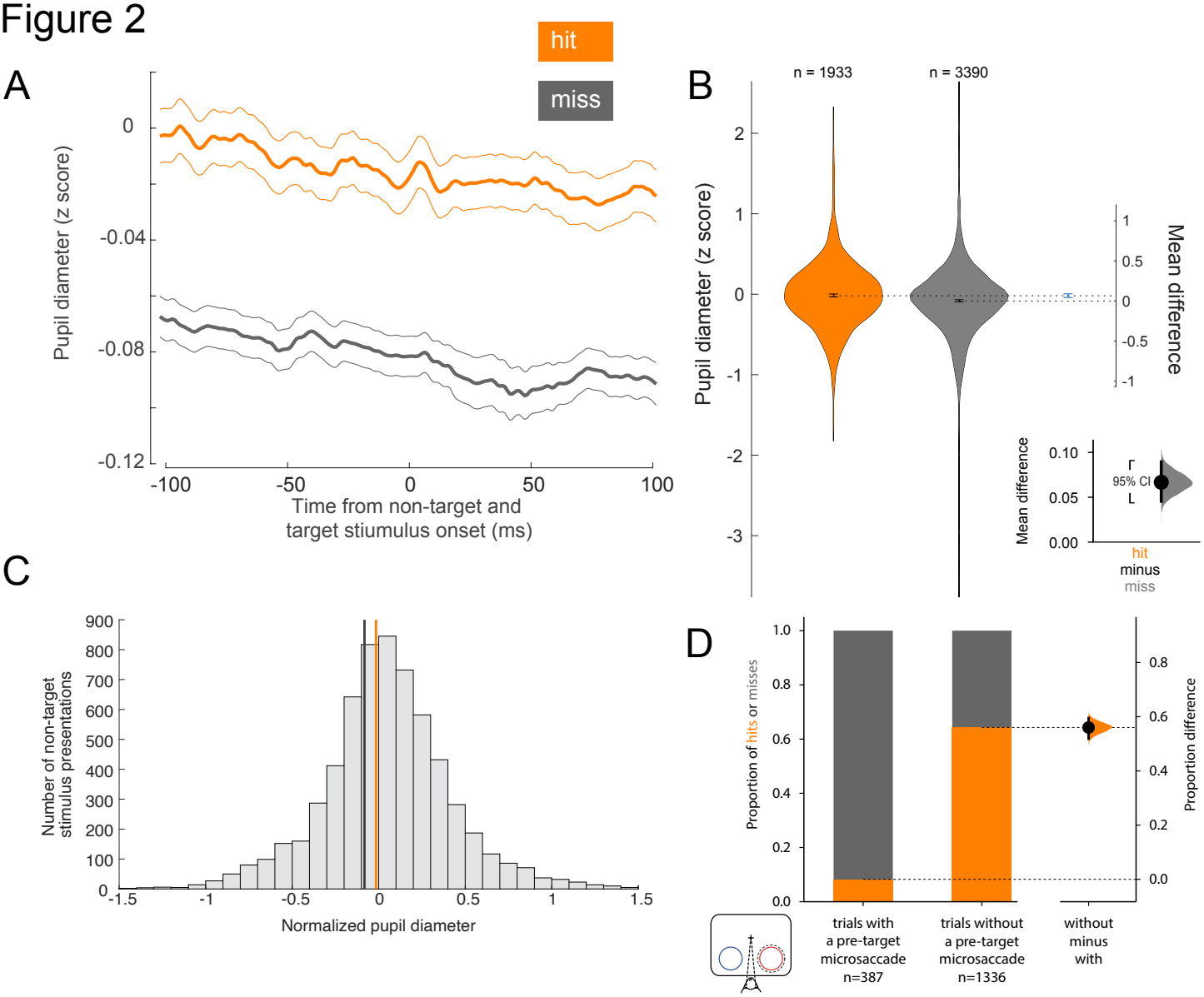

Figure 2. Hit trials have larger pupil diameter whereas microsaccades more often precede misses
(**A**) Normalized pupil diameter for hit and miss trails in the threshold condition. 0 ms corresponds to non-target and target stimulus onset. Mean +/- s.e.m. (**B**) Distribution of pupil diameter values associated with hit and miss trials. Pupil diameter was averaged from 100ms before to 100ms after non-target and target stimulus onset. Violin plots were generated using kernel smoothing (See Experimental Procedures). Error bars represent 95% confidence intervals for the mean of each distribution, and the mean difference (blue, right axes). Inset: zoomed in view of the mean difference between hit and miss trials. Black bar represents a 95% confidence interval of the mean difference. Shaded region reflects the distribution of the bootstrapped estimation of the mean difference. (**C**) Histogram of mean pupil diameter around the time of non-target and target stimulus onset (calculated as in **B**). Orange and gray lines represent the mean pupil diameter for hit and miss trials respectively. (**D**) *Left:* Hit rate for trials with (387 trials) and without (right, 1336 trials) a microsaccade detected in the time window 0-400ms before target onset. *Right:* Bootstrapped estimation of the mean difference in hit proportion in trials with vs without a pre-target microsaccade. Same conventions as **2B**.

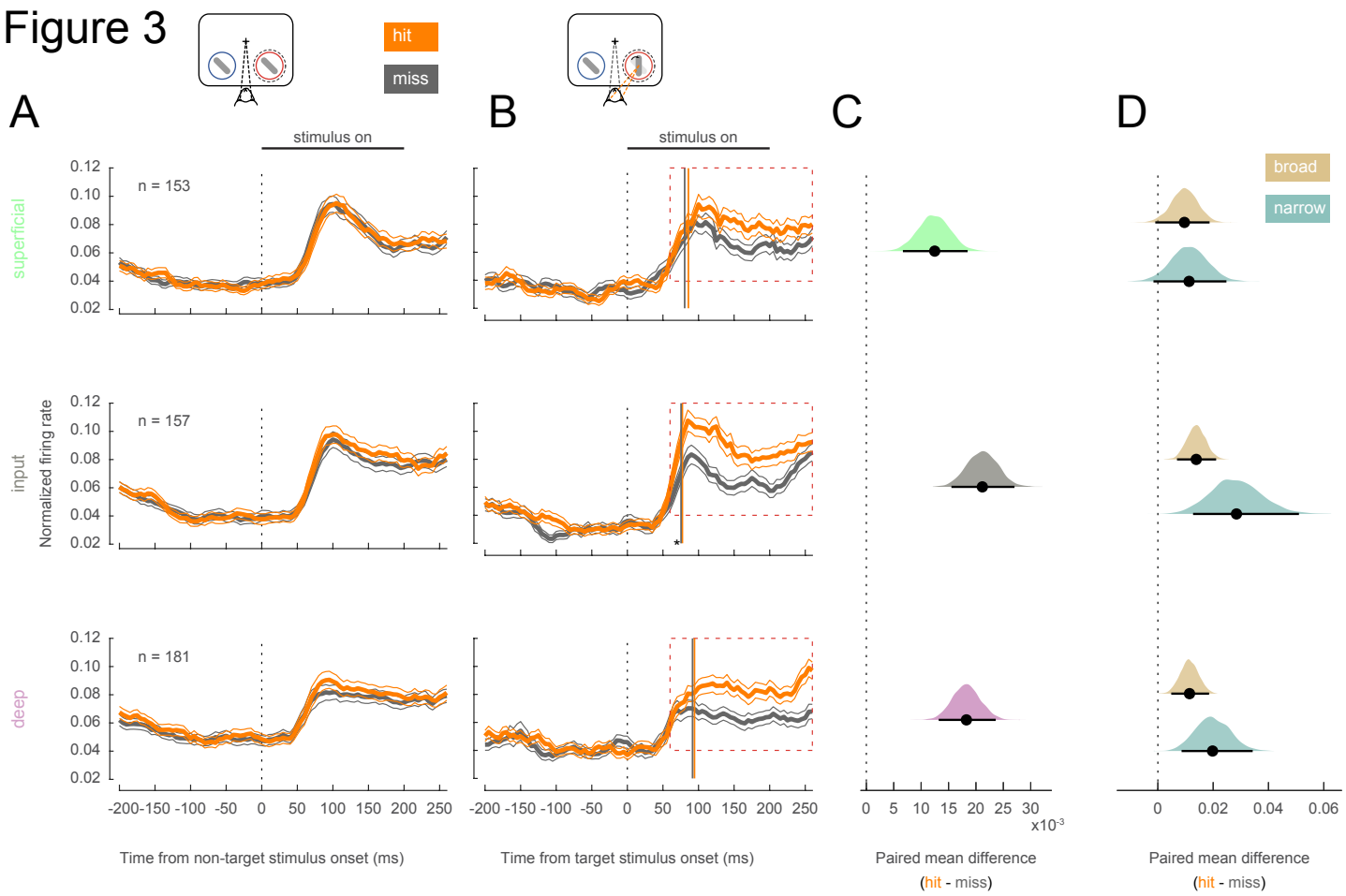

Figure 3. Target stimuli evoke higher firing rates in hit trials
Rows correspond to different layers (top=superficial, middle=input, bottom=deep). (**A**) Non-target population (single and multi-unit) non-target PSTH of visually responsive neurons for the hit (orange) and miss (dark-gray) trials in the threshold condition (mean +/- s.e.m). The horizontal black bar indicates the time and duration of stimulus presentation. (**B**) As in **A** but for target stimuli. The star indicates the time at which firing rates in the input layer first differ significantly between hit and miss trials. Vertical lines represent the mean time firing rates for each neuron rise above the 95% confidence interval of their baseline activity (see also Figure S3C). (**C**) Bootstrapped estimation of the paired mean difference in target stimulus-evoked firing rate across hit and miss trials in the time window 60-260ms (red dotted box in **B**) after target stimulus onset. Shaded regions represent the bootstrapped estimation of the paired mean difference in firing rate (hit - miss), and black lines are 95% confidence intervals. Plots include data from both single and multi-units, separated by layer (top= superficial, middle=input, bottom=deep). (**D**) As in **C**, bootstrapped estimation of the paired mean difference in firing rate for hit trials compared to miss trials in the target stimulus-evoked period, but only for single-units broken up by cell class (gold=broad, teal=narrow).

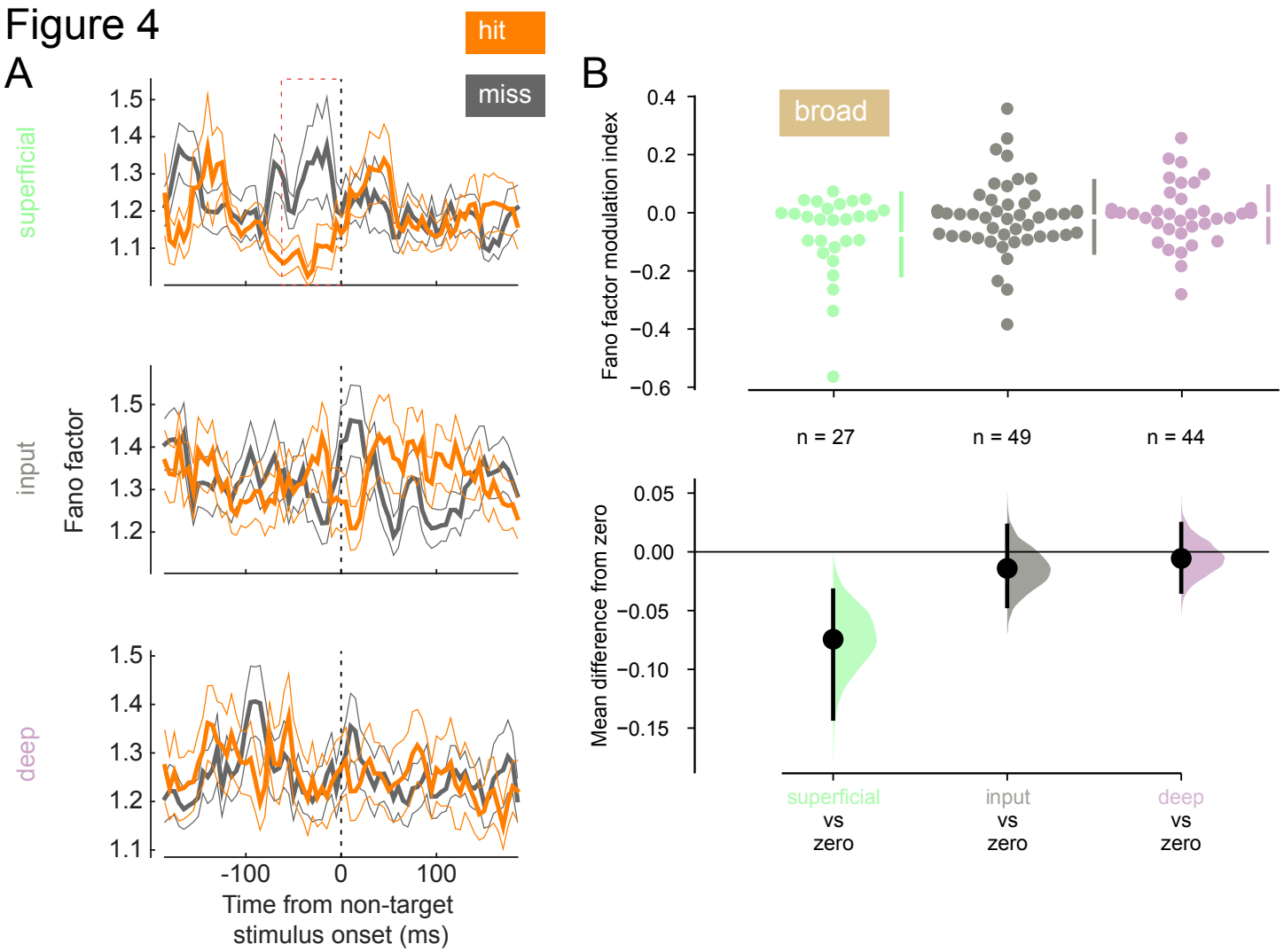

Figure 4. Broad-spiking neurons in the superficial layer have decreased variability in hit trials
(**A**) Rows correspond to different layers (top=superficial, middle=input, bottom=deep). The Fano factor of broad-spiking putative excitatory neurons for the hit and miss trials in the threshold condition (mean +/- s.e.m). There is a significant decrease in variability for the hit trials prior to stimulus onset only in the superficial layer. 0 ms corresponds to non-target stimulus onset. The average Fano factor within a 60ms time-window (red dashed box) prior to stimulus onset is plotted in **B**. (**B**) *Top:* Fano factor modulation index for each broad-spiking neurons recorded in each layer, averaged in the 60ms preceding non-target stimulus onset. *Bottom:* Bootstrapped estimation of the mean difference of the Fano factor modulation index from zero in each of the three layers. Colored curves represent the estimated bootstrapped distribution. Black dots and lines reflect the mean and 95% confidence intervals of the distributions.

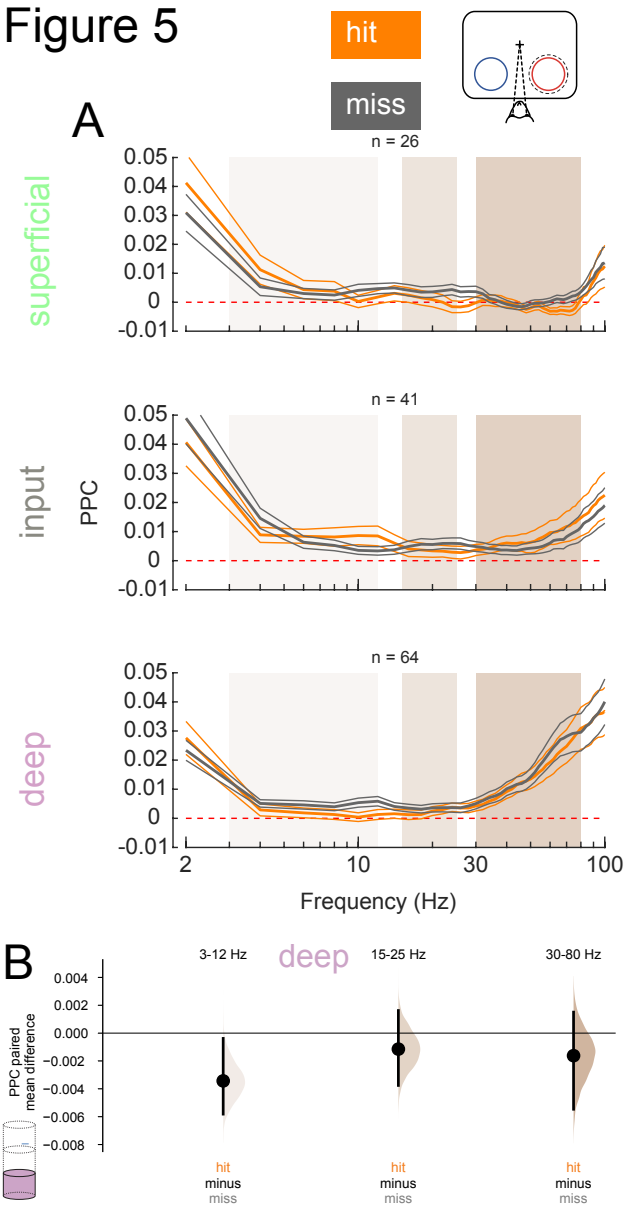

Figure 5. Deep layer neurons are phase-locked to low-frequency rhythms in miss trials
(**A**) Pairwise phase consistency (PPC) of single and multi-units in each layer to the local field potential (LFP) signal recorded from the same channel in hit and miss trials at threshold. PPC was calculated in the pre-stimulus period (0-200 ms before stimulus onset). Dashed red line indicates a PPC of 0, below which there is no consistent relationship between spikes and LFP phase. (**B**) Bootstrapped estimation plot for the paired mean difference in PPC for deep layer neurons over three frequency bands: 3-12Hz, 15-25Hz, 30-80Hz. Curves represent the bootstrapped distribution for the paired difference, and black dots and vertical lines represent the mean and 95% confidence intervals for the paired mean difference

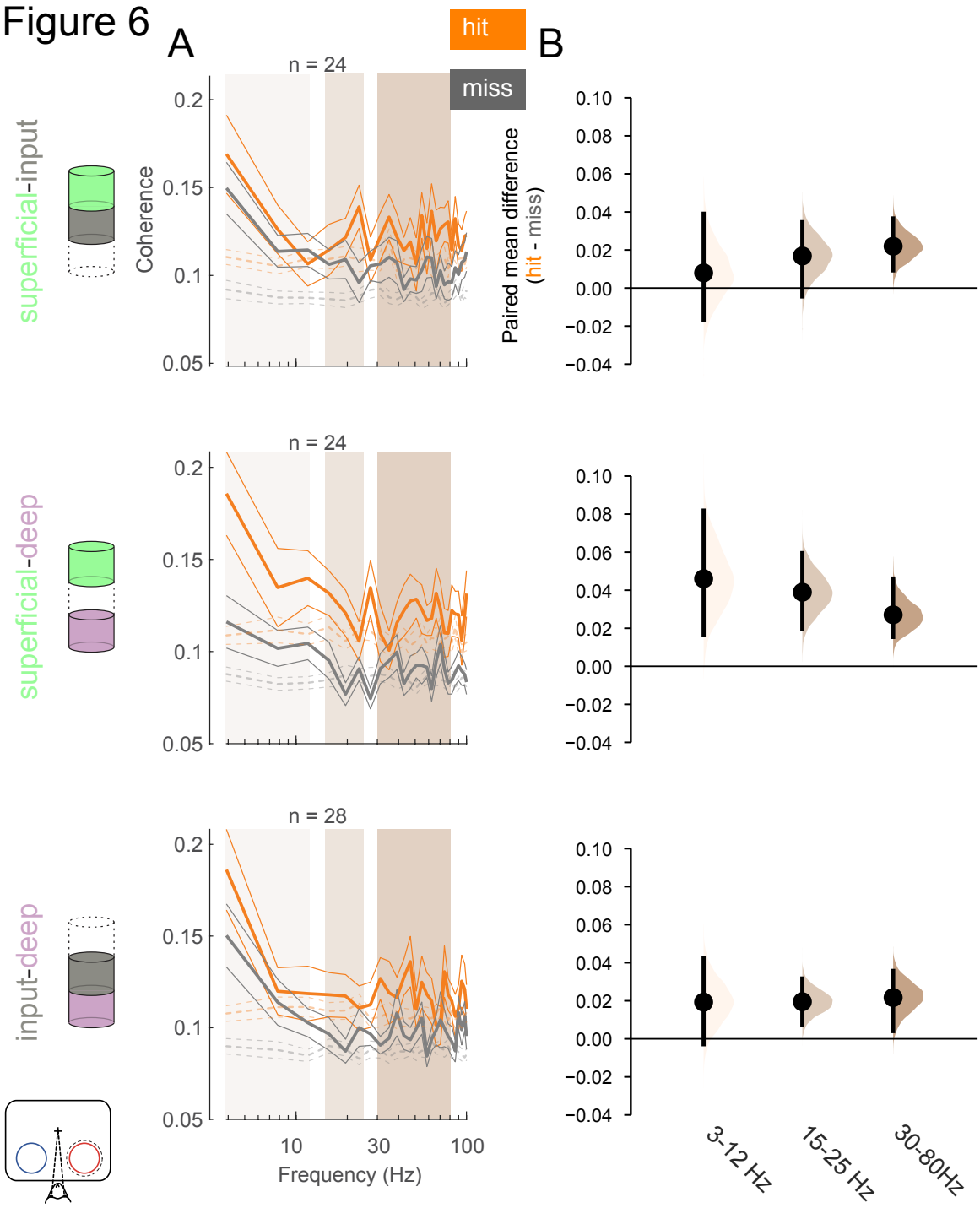

Figure 6. Greater interlaminar coherence in hit trials in the pre-stimulus period
Interlaminar spike-spike coherence in the pre-stimulus period (0-200ms prior to stimulus onset). Rows correspond to different pairs of layers (*top*=superficial-input, *middle*=superficial-deep, *bottom*=input-deep). (**A**) Multi-unit interlaminar spike-spike coherence (SSC) calculated in the 200ms before non-target stimulus onset in hit and miss trials (solid lines, mean +/- s.e.m). Firing rates were matched across hit and miss trials. Dashed lines represent coherence calculated with shuffled trial identities (mean +/- s.e.m). (**B**) Bootstrapped estimation plot for the paired mean difference in SSC for each pair of layers averaged over three frequency bands : 3-12Hz, 15-25Hz, 30-80Hz. Curves represent the bootstrapped distribution for the paired difference, and black dots and vertical lines represent the mean and 95% confidence intervals for the paired mean difference.

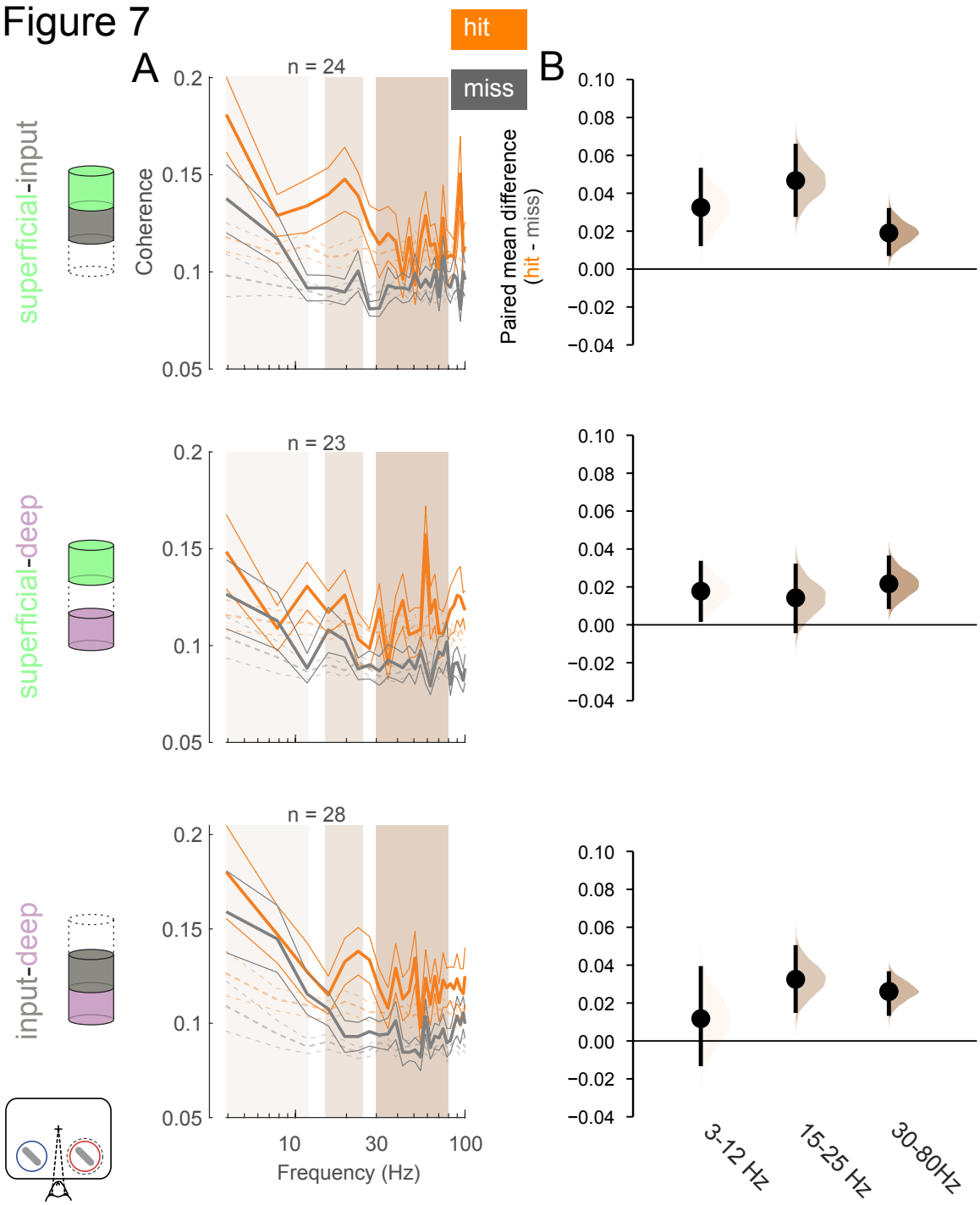

Figure 7. Greater interlaminar coherence in hit trials in the non-target stimulus-evoked period
Interlaminar spike-spike coherence in the non-target stimulus evoked period (60-260ms after stimulus onset). Same conventions as in Figure 6.

Figure 8

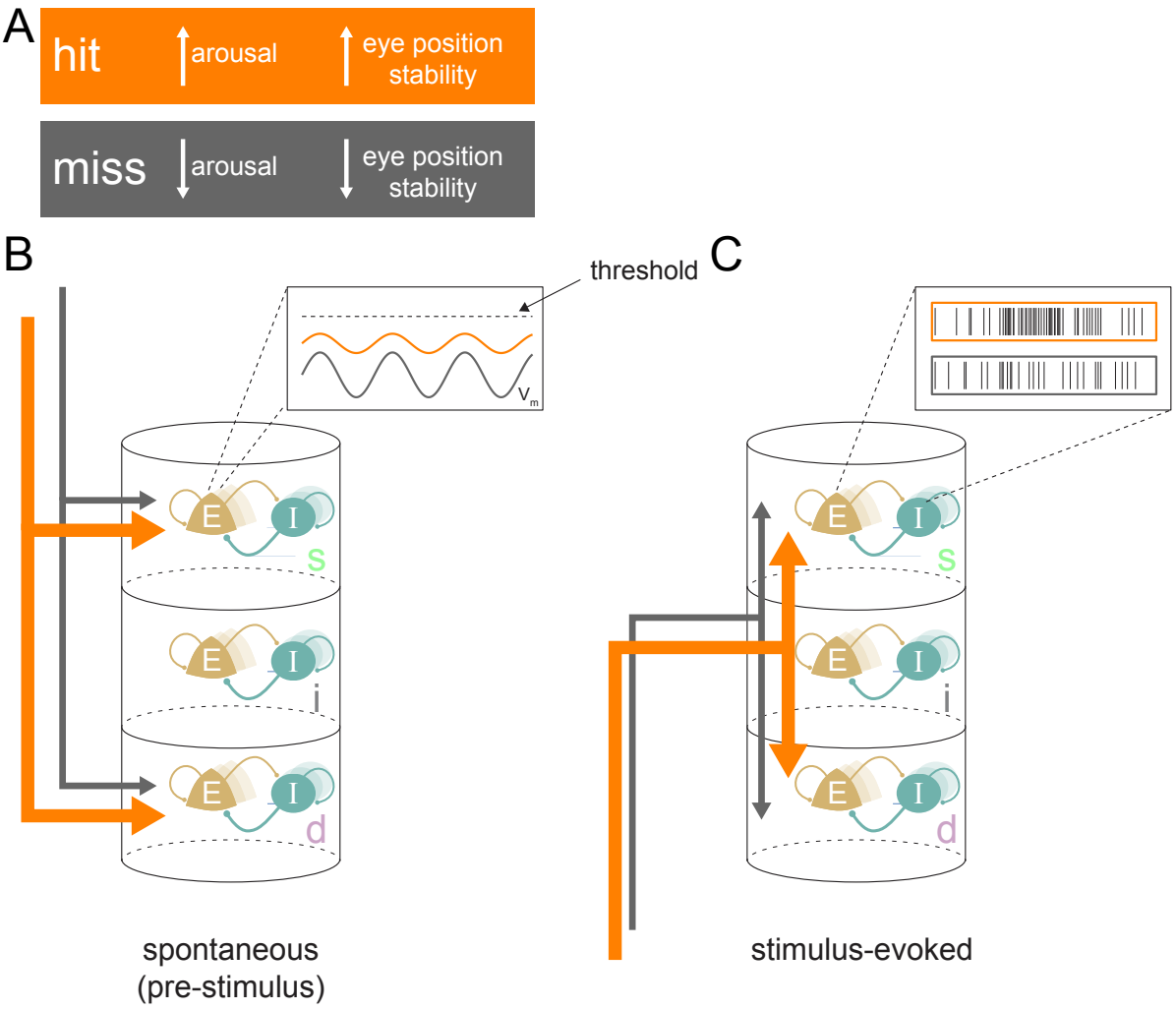

Figure 8. Conceptual model for stimulus processing at perceptual threshold
(**A**) Hit trials have a larger pupil diameter and fewer pre-target microsaccades, reflecting a state of increased arousal and greater eye position stability. Conversely, miss trials show decreased arousal and eye position stability. (**B**) In the spontaneous pre-stimulus period, hits are characterized by decreased variability in superficial layer broad-spiking neurons, which we hypothesize is reflective of lower membrane potential (V_m) variability (inset). Hit trials are also characterized by greater synchrony between the superficial and deep layers (indicated by thicker arrows), which could be reflecting a stronger top-down influence on the cortical column. (**C**) In the stimulus-evoked period there is greater interlaminar synchrony between pairs that include the input layer (represented by thicker arrows), which we propose reflects improved feed-forward propagation of information. We propose these state differences in hits contribute to elevated firing rates in response to target stimuli, particularly in the superficial layers (inset), resulting in a higher-fidelity output to downstream areas. E = excitatory; I = inhibitory; s = superficial; i = input; d = deep.

Figure 1-figure supplement 1

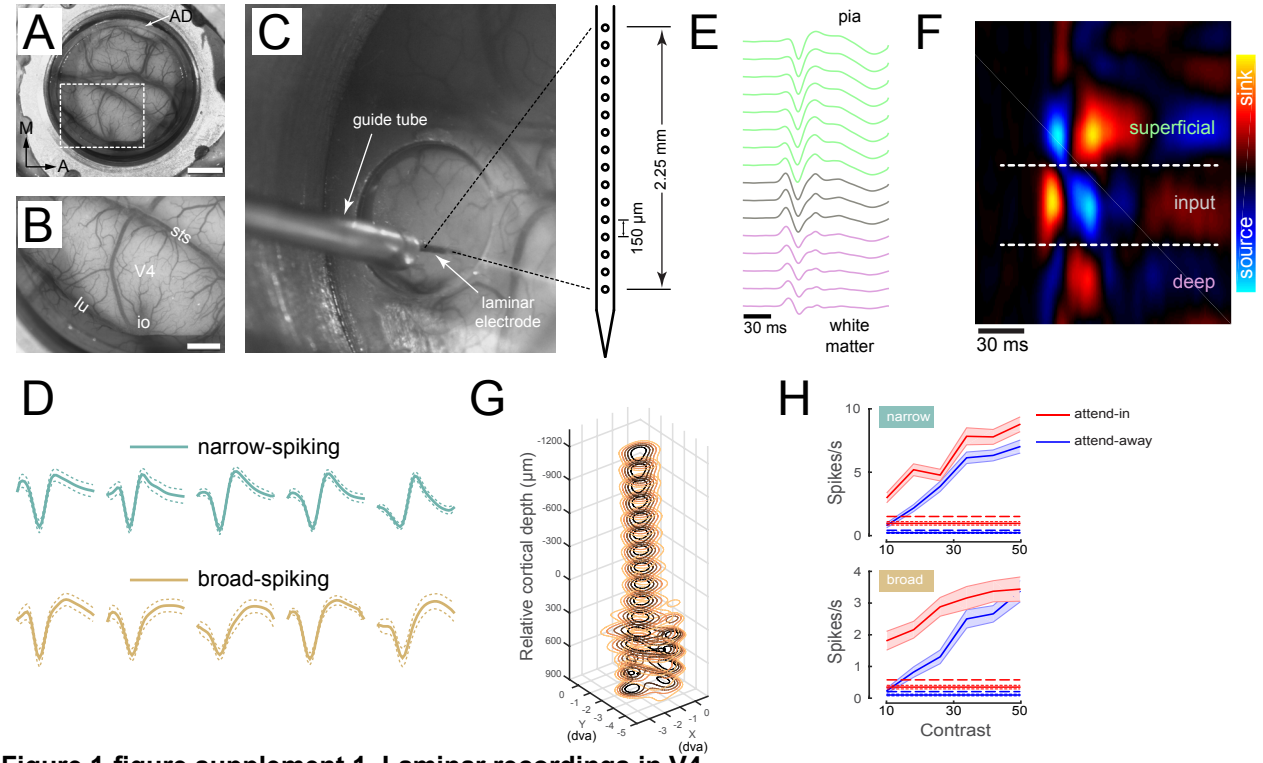

Figure 1-figure supplement 1. Laminar recordings in V4

(**A**) An artificial dura (AD) chamber is shown over dorsal V4 in the right hemisphere of Monkey A. The native dura mater was resected and replaced with a silicone based artificial dura, thereby providing an optically clear window into the cortex. Scale bar = 5mm. (**B**) An enlarged view of the boxed region in **A** clearly shows the sulci and the microvasculature. sts = superior temporal sulcus, lu = lunate sulcus, io = inferior occipital sulcus. Area V4 lies on the pre-lunate gyrus between the superior temporal and lunate sulci. Scale bar = 2mm. (**C**) Electrophysiology setup: a plastic stabilizer with a circular aperture is secured in place inside the chamber such that the aperture is centered over the pre-lunate gryus. A 16-channel linear array electrode (electrode spacing 150m) is positioned over the center of the gyrus and lowered into the cortex under microscopic guidance. The microvasculature pattern was used as a reference to target different cortical sites across recording sessions. (**D**) Example recording session in monkey C depicting 12 single unit waveforms (mean +/- s.e.m.) isolated along the cortical column. Teal waveforms correspond to narrow-spiking putative interneurons and gold waveforms correspond to broad-spiking putative excitatory units. (**E**) Stimulus triggered local field potentials (LFPs) obtained by flashing 30ms high contrast ring stimuli in the receptive field of a V4 cortical column. LFP traces averaged across all stimulus repeats are shown color-coded as being part of either the superficial (green), input (gray) or deep (pink) layers. Layer assignment was done after current source-density analysis. (**F**) Current source-density (CSD) calculated as the second spatial derivative of the stimulus triggered LFPs and displayed as a colored map. The x-axis represents time from stimulus onset; the y-axis represents cortical depth oriented such that the pial surface is at the top and the white matter is at the bottom. Red hues represent current sink, blue hues represent current source. The input layer is identified as the first current sink followed by a reversal to current source. The superficial and deep layers have the opposite sink-source pattern. The CSD map has been spatially smoothed for visualization. (**G**) Stacked contour plots show spatial receptive fields (RFs) mapped along each contact point in the laminar probe. The spatial receptive fields were obtained by applying reverse correlation to the LFP power evoked by sparse pseudo-random sequences of Gabor stimuli. The RFs are well aligned, indicating perpendicular penetration down a cortical column. Zero depth represents the center of the input layer as estimated from the CSD. (**H**) Contrast response functions – spikes rate as a function of stimulus contrast – are shown for 2 example units identified in a single recording session in Monkey A. Red and blue traces correspond to the attend-in to RF and attend-away from RF conditions respectively. The dotted lines represent the corresponding background firing-rates. The dashed lines are 4 standard deviations above baseline. A unit was considered as visually responsive, if the contrast response functions exceeded this threshold in both the attention conditions. Mean +/- s.e.m.

Figure 2-figure supplement 1

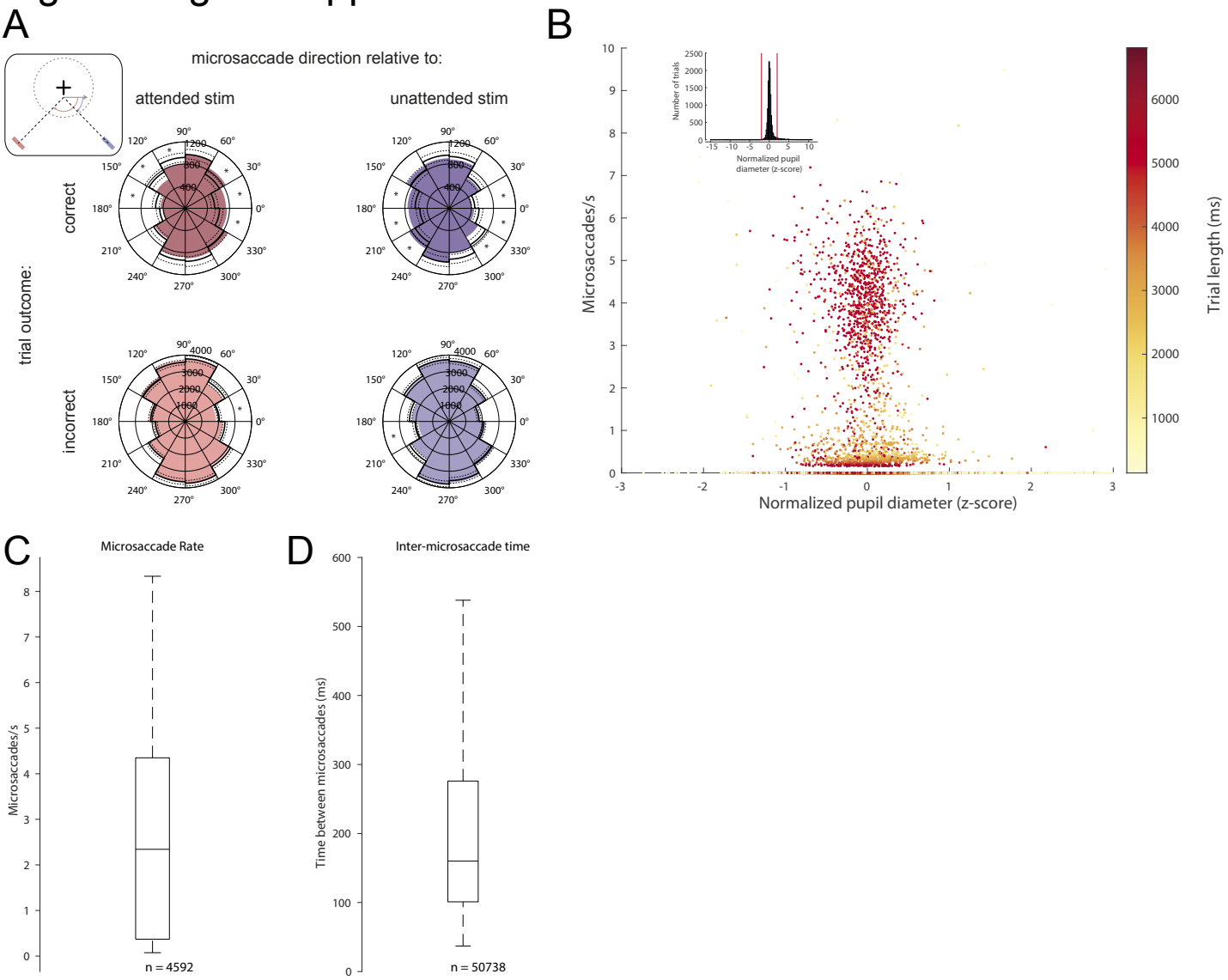

Figure 2-figure supplement 1. Microsaccades are preferentially directed towards the target in correct trials and have a slight correlation with pupil diameter

Data is presented for all trials, regardless of orientation change (not just the threshold condition). (**A**) The histograms represent the direction of microsaccades relative to the attended stimulus (left column) or unattended stimulus (right column) in correct (top row) and incorrect (bottom row) trials. Black lines represent the mean (solid) and 99.5% confidence interval (dashed) of the bootstrapped null distribution estimated by pooling correct and incorrect microsaccades. . *Inset:* Schematic for calculation of relative microsaccade direction. Microsaccade is represented by the gray arrow (**B**) Scatterplot of microsaccade rate versus mean normalized pupil diameter, shows a small but statistically significant relationship between the two quantities (r^2 = 0.006, p<0.001). Each dot is color-coded by trial length. *Inset:* Histogram of mean pupil diameter for all trials, including those less than -2 or greater than 2 (red lines). Only four of the trials with pupil diameters less than -2 or greater than 2 had detected microsaccades. (**C**) Boxplot of microsaccade rates for all trials. (**D**) Boxplot of the time between microsaccades recorded in the same trial. 4% of microsaccades separated by more than 538ms were excluded as outliers (See Methods).

Figure 3-figure supplement 1

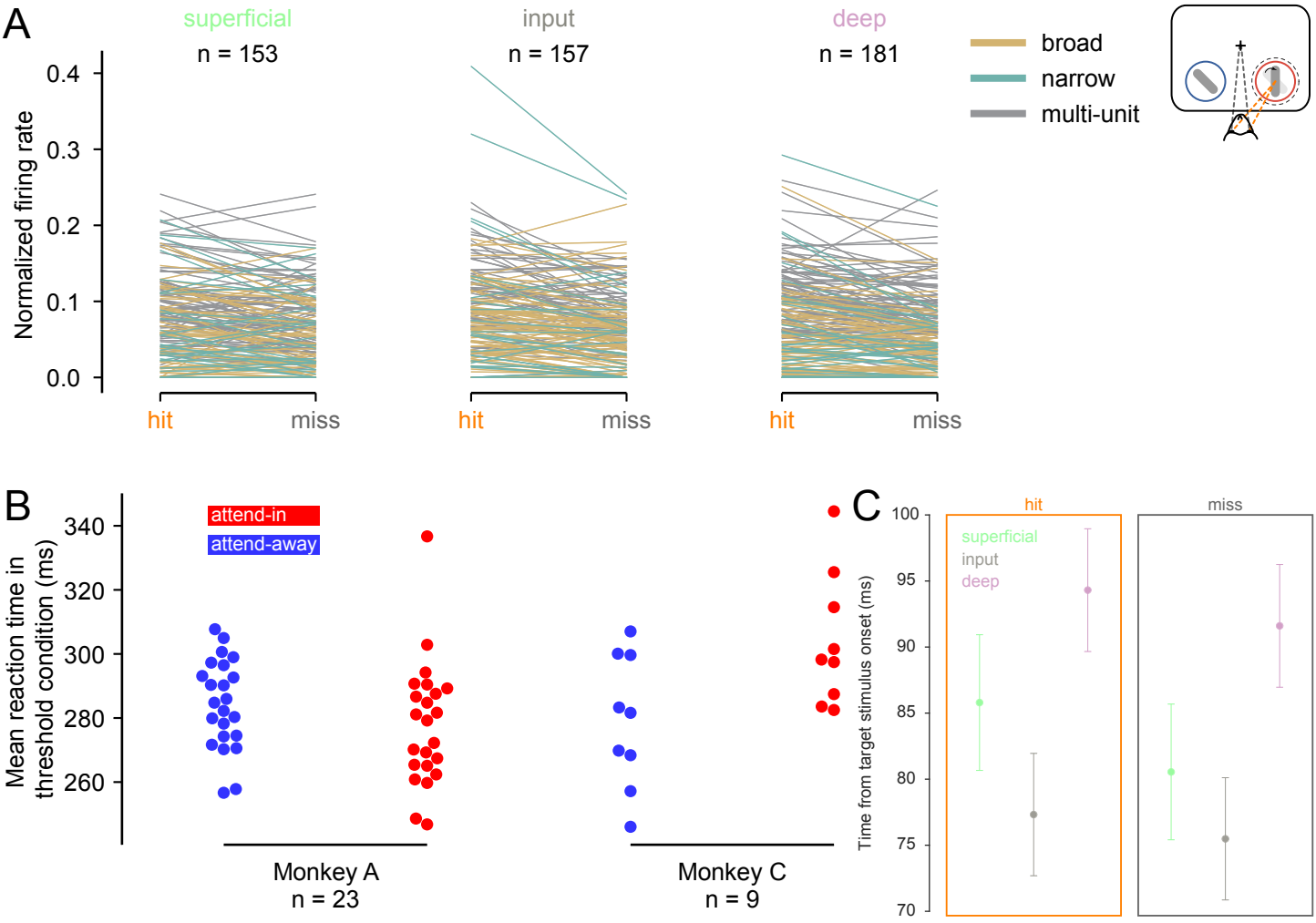

Figure 3-figure supplement 1. Firing rates for individual neurons and reaction time in threshold condition
(**A**) Target stimulus-evoked normalized firing rates in hit and miss trials for each recorded single and multi-unit cluster in hit and miss trials. Clusters are divided by layer: left=superficial, middle=input, right=deep. Related to Figure 3B. Each line represents the mean firing rate in response to target stimuli in hit and miss trials for a given unit. Data is color coded by unit type (gold=broad, teal=narrow, gray=multi-unit). See Experimental Procedures for normalization method. (**B**) Mean reaction time in response to the target stimulus in the threshold condition in both attend-in (red) and attend-away (blue) trials for each recording session. (**C**) Mean time at which single- and multi-unit firing rates rise significantly above pre-stimulus baseline in response to target stimuli in hit and miss trials. Mean +/- s.e.m.

Figure 4-figure supplement 1

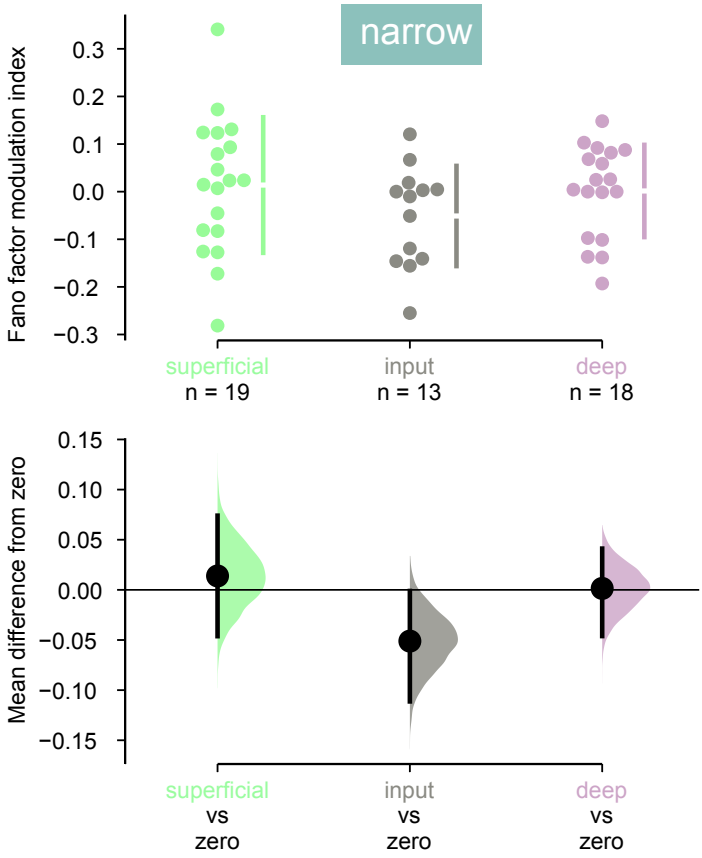

Figure 4-figure supplement 1. Narrow-spiking neurons do not have decreased variability in hit trials
Top: Fano factor modulation index for each narrow-spiking neurons recorded in each layer, averaged in the 60ms preceding non-target stimulus onset. *Bottom*: Bootstrapped estimation of the mean difference of the Fano factor modulation index from zero in each of the three layers. Colored curves represent the estimated bootstrapped distribution. Black dots and lines reflect the mean and 95% confidence intervals of the distributions.

Figure 5-figure supplement 1

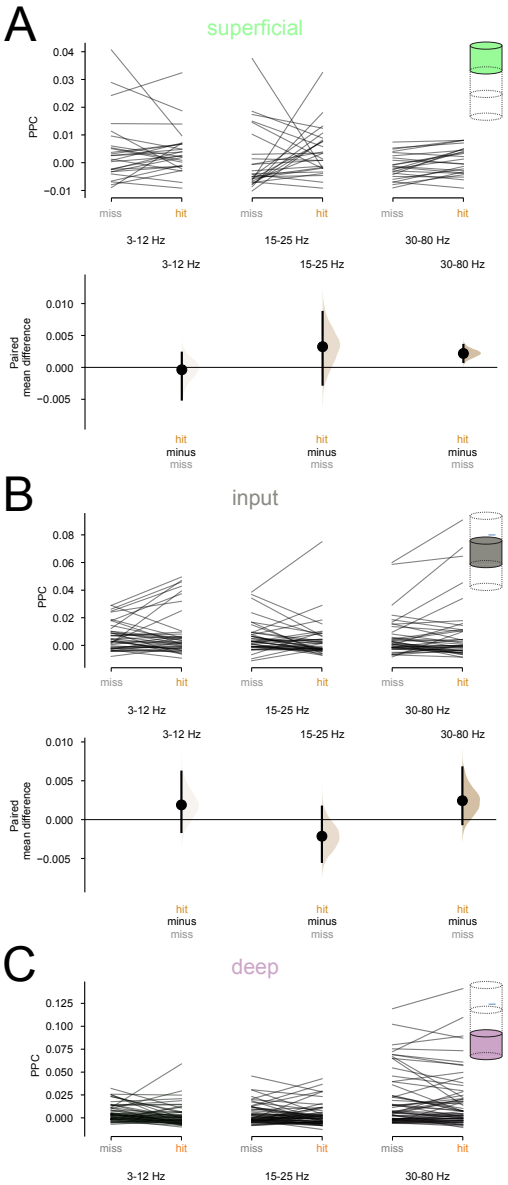

Figure 5-figure supplement 1. Additional PPC data
(**A-B**) *Top:* Raw PPC values calculated for clusters recorded in the superficial (**A**) and (**B**) input layers in hit and miss trials, averaged into three frequency bands, 3-12 Hz, 15-25 Hz, and 30-80 Hz. PPC was calculated using the LFP recorded on the same channel as the spikes. *Bottom:* Bootstrapped estimation of the paired mean difference in PPC across hit and miss trials for each frequency band. Note that although there appears to be a difference in high-frequency PPC in the superficial layer, this population does not have significantly positive PPC in either condition, indicating that there is no phase-locking in either hits or misses. (**C**) Raw PPC values for neurons recorded in the deep layer in hit and miss trials, averaged into the same 3 frequency bands. Related to Figure 5B.

Table 1: Corresponding Null-Hypothesis Testing Results

Figure	Null-Hypothesis Test	P-Value
2B (pupil diameter)	*t*-test (unpaired)	$p = 6.63624\text{e} - 09$
2D (microsaccades)	X^2-test	$p \ll 0.0001$
3B (target-evoked firing rate, single and multi-units)	*t*-test (paired) Bonferoni Corrected for 3 comparisons, $\alpha = 0.0166$	Superficial: $p = 4.19108\text{e} - 05$ Input: $p = 1.10838\text{e} - 11$ Deep: $p = 1.75826\text{e} - 11$
3C (target-evoked firing rate, broad-spiking)	*t*-test (paired) Bonferoni Corrected for 3 comparisons, $\alpha = 0.0166$	Superficial: $p = 0.0526902$ Input: $p = 0.000124947$ Deep: $p = 0.00119012$
3C (target-evoked firing rate, narrow-spiking)	*t*-test (paired) Bonferoni Corrected for 3 comparisons, $\alpha = 0.0166$	Superficial: $p = 0.103689$ Input: $p = 0.00570757$ Deep: $p = 0.00393437$
4B (Fano Factor modulation index, broad)	*t*-test (unpaired) Bonferoni Corrected for 3 comparisons, $\alpha = 0.0166$	Superficial: $p = 0.0102155$ Input: $p = 0.418197$ Deep: $p = 0.708115$
S4 (Fano factor modulation index, narrow)	*t*-test (unpaired) Bonferoni Corrected for 3 comparisons, $\alpha = 0.0166$	Superficial: $p = 0.676039$ Input: $p = 0.10532$ Deep: $p = 0.950487$
5B (deep PPC)	*t*-test (paired) Bonferoni Corrected for 3 comparisons, $\alpha = 0.0166$	3-12 Hz: $p = 0.0142$ 15-25 Hz: $p = 0.4064$ 30-80 Hz: $p = 0.3600$
6B (top, superficial-input SSC modulation index)	*t*-test Bonferoni Corrected for 3 comparisons, $\alpha = 0.0166$	3-12 Hz: $p = 0.925338$ 15-25 Hz: $p = 0.107304$ 30-80 Hz: $p = 0.00394525$
6B (middle, superficial-deep SSC modulation index)	*t*-test Bonferoni Corrected for 3 comparisons, $\alpha = 0.0166$	3-12 Hz: $p = 0.0125919$ 15-25 Hz: $p = 0.00116552$ 30-80 Hz: $p = 0.00142568$
6B (bottom, input-deep SSC modulation index)	*t*-test Bonferoni Corrected for 3 comparisons, $\alpha = 0.0166$	3-12 Hz: $p = 0.260698$ 15-25 Hz: $p = 0.0358178$ 30-80 Hz: $p = 0.0325516$
7B (top, superficial-input SSC modulation index)	*t*-test Bonferoni Corrected for 3 comparisons, $\alpha = 0.0166$	3-12 Hz: $p = 0.00344279$ 15-25 Hz: $p = 3.17111\text{e} - 05$ 30-80 Hz: $p = 0.00396824$
7B (middle, superficial-deep SSC modulation index)	*t*-test Bonferoni Corrected for 3 comparisons, $\alpha = 0.0166$	3-12 Hz: $p = 0.0164846$ 15-25 Hz: $p = 0.0890114$ 30-80 Hz: $p = 0.00441928$
7B (bottom, input-deep SSC modulation index)	*t*-test Bonferoni Corrected for 3 comparisons, $\alpha = 0.0166$	3-12 Hz: $p = 0.241036$ 15-25 Hz: $p = 0.00140176$ 30-80 Hz: $p = 6.84271\text{e} - 05$
5-supplement 1B (superficial PPC)	*t*-test (paired) Bonferoni Corrected for 3 comparisons, $\alpha = 0.0166$	3-12 Hz: $p = 0.8307$ 15-25 Hz: $p = 0.2812$ 30-80 Hz: $p = 0.0037$*
5-supplement 1C (input PPC)	*t*-test (paired) Bonferoni Corrected for 3 comparisons, $\alpha = 0.0166$	3-12 Hz: $p = 0.3440$ 15-25 Hz: $p = 0.2517$ 30-80 Hz: $p = 0.1881$

* Although this p-value is significant, the PPC in both conditions is below 0, indicating there is no phase-locking in either condition (Vinck et al., 2010).

Table 2: GLM Values

Variable (Z-Scored)	Estimated Coefficient	P-Value
Pupil Diameter	0.11754	$p = 0.32869$
Pretarget Microsaccades	-1.3116	$p = 6.0757e - 08$
Target Superficial FR	0.22414	$p = 0.091946$
Target Input FR	0.3276	$p = 0.020068$
Target Deep FR	0.11399	$p = 0.45762$