

Algorithms for Estimating Time-Locked Neural Response Components in Cortical Processing of Continuous Speech

Joshua P. Kulasingham and Jonathan Z. Simon

Abstract— Objective: The Temporal Response Function (TRF) is a linear model of neural activity time-locked to continuous stimuli, including continuous speech. TRFs based on speech envelopes typically have distinct components that have provided remarkable insights into the cortical processing of speech. However, current methods may lead to less than reliable estimates of single-subject TRF components. Here, we compare two established methods, in TRF component estimation, and also propose novel algorithms that utilize prior knowledge of these components, bypassing the full TRF estimation. **Methods:** We compared two established algorithms, ridge and boosting, and two novel algorithms based on Subspace Pursuit (SP) and Expectation Maximization (EM), which directly estimate TRF components given plausible assumptions regarding component characteristics. Single-channel, multi-channel, and source-localized TRFs were fit on simulations and real magnetoencephalographic data. Performance metrics included model fit and component estimation accuracy. **Results:** Boosting and ridge have comparable performance in component estimation. The novel algorithms outperformed the others in simulations, but not on real data, possibly due to the plausible assumptions not actually being met. Ridge had slightly better model fits on real data compared to boosting, but also more spurious TRF activity. **Conclusion:** Results indicate that both smooth (ridge) and sparse (boosting) algorithms perform comparably at TRF component estimation. The SP and EM algorithms may be accurate, but rely on assumptions of component characteristics. **Significance:** This systematic comparison establishes the suitability of widely used and novel algorithms for estimating robust TRF components, which is essential for improved subject-specific investigations into the cortical processing of speech.

Index Terms — MEG, EEG, auditory, deconvolution, reverse correlation, attention, cocktail party, matching pursuit, ERP

I. INTRODUCTION

THE human brain time-locks to features of continuous speech, extracting meaningful information relevant to comprehension. Magnetoencephalography (MEG) and electroencephalography (EEG) are suitable methods to measure these time-locked responses, due to their high temporal resolution. Traditional methods for analyzing auditory responses involve averaging over multiple trials of repeated stimuli to estimate Evoked Response Potentials (ERPs) [1], [2]. But exploring the complex mechanisms involved in speech processing requires non-repetitive, continuous speech stimuli of long duration, and averaging over trials is no longer feasible. One method of analyzing responses to continuous stimuli uses linear models called Temporal Response Functions (TRFs), that estimate the impulse response of the neural system to continuous stimuli [3], [4]. TRFs based

This work was supported by the National Science Foundation (SMA-1734892), and the National Institutes of Health (R01-DC014085 and R01-DC019394). J. P. Kulasingham is with the Department of Electrical and Computer Engineering, University of Maryland, College Park, MD, USA. (joshuapk@terpmail.umd.edu)
J. Z. Simon is with the Department of Electrical and Computer Engineering, the Institute for Systems Research, and the Department of Biology, University of Maryland, College Park, MD, USA.

27 on neural recordings using magnetoencephalography (MEG) have response components such as the M50 (~50 ms latency),
28 M100 (~100-150 ms) and M200 (~200-250 ms) that are analogous to well-known auditory ERP components, the P1, N1, and P2
29 components of electroencephalography (EEG), and which have been utilized to investigate selective attention [3], [5]–[7],
30 linguistic processing [8]–[10], and age-related differences in the auditory system [11]. However, though estimated TRFs display
31 these canonical components at the group-average level, individual TRFs are much noisier and do not always have well-defined
32 components. It is essential to detect robust response components on a per-subject level, both to identify task effects and for
33 biomedical applications such as smart hearing aids. Hence, the suitability of various TRF methods for component estimation
34 must be determined.

35 Variations of regularized regression and machine learning methods for estimating TRFs have been previously compared for
36 decoding subject attention in a multi-talker scenario [6], [12], [13]. However, it is unclear how they compare to commonly used
37 sparse TRF estimation techniques such as boosting [14], [15]. Furthermore, a focus on model fits for attention decoding may not
38 be suitable for studies interested in accurate estimation of TRF components.

39 In this work we perform a systematic comparison of TRF algorithms in terms of estimating TRF components. Two widely
40 used TRF estimation algorithms are ridge regression [13], [16] and boosting [3], [14], [15]. The former uses ℓ_2 regularization
41 which leads to smooth TRFs with broad components, while the latter greedily adds values to the TRF, thereby prioritizing
42 sparsity in the TRF and leading to narrower, sharper components. However, it is not clear which of these methods is more
43 accurate in estimating TRF component latencies and amplitudes.

44 Both ridge and boosting do not place restrictions on the number or latencies of specific TRF components. Since canonical
45 auditory response components are often present in TRFs to the speech envelope, it is reasonable to incorporate this information
46 during estimation. Several methods have been proposed for directly estimating latencies and amplitudes for M/EEG evoked
47 responses (but not for TRFs). The earliest ERP latency estimation methods involved cross correlation with average response
48 templates [17]. More recent algorithms have utilized techniques such as Independent Component Analysis [18], [19], wavelet
49 decomposition [20], maximum likelihood estimation [21], [22], autoregressive models [23], Expectation Maximization (EM)
50 [24], Matching Pursuit [25] and Bayesian methods [26], [27].

51 In this work, we propose novel TRF component estimation algorithms that utilize prior knowledge of the characteristics of
52 neural responses (i.e., component latency ranges), and directly estimate component latencies, amplitudes and topographies. The
53 first proposed algorithm estimates single-channel TRF component latencies and amplitudes using Subspace Pursuit (SP) [28].
54 The second algorithm extends this method for multi-channel TRFs using SP and Expectation Maximization (EM) [24], [29], and
55 also directly estimates sensor topographies or cortical source distributions of TRF components. The SP algorithm is widely used
56 for sparse signal recovery and is typically capable of recovering components in an efficient manner. The EM algorithm is a
57 maximum likelihood method that is able to incorporate ‘hidden’ variables and is widely used in signal estimation [30]. Pursuit
58 algorithms and EM have been used for single trial evoked response estimation [24], [25], and here, we employ natural extensions
59 of these algorithms for TRF component estimation.

60 A simulation study, and an application of these algorithms to a real dataset, are reported and their performance is compared
61 using single-channel, multi-channel, and source localized TRFs. Performance metrics include the correlation between the actual
62 and the predicted signal, which is the conventional measure of model fit, and several other measures of component estimation
63 accuracy. Throughout this work, “model fit” denotes the Pearson correlation between the actual and predicted signals. Other
64 considerations such as spurious TRF activity and missing components are also examined. In summary, this work discusses the
65 strengths and weaknesses of widely used algorithms and proposes novel methods for TRF component estimation that may
66 provide robust and interpretable time-locked response components.

67 II. METHODS

68 A. Established Algorithms for TRF estimation

69 The TRF estimation problem is given by the convolution

$$\mathbf{y} = \boldsymbol{\beta} * \mathbf{x} + \mathbf{n} \quad (1)$$

70 Where $\mathbf{y} \in \mathbb{R}^T$ is the vector of the single-channel measured signal (e.g., at one sensor) for T time points, $\mathbf{x} \in \mathbb{R}^T$ is the
71 predictor variable (e.g., the speech envelope), $\boldsymbol{\beta} \in \mathbb{R}^K$ is the corresponding TRF over K time lags, and $\mathbf{n} \in \mathbb{R}^T$ is the noise. This
72 can be reformulated as a regression as follows

$$\mathbf{y} = \mathbf{X}\boldsymbol{\beta} + \mathbf{n} \quad (2)$$

73 Where $\mathbf{X} \in \mathbb{R}^{T \times K}$ is the Toeplitz matrix formed by lagged predictor values. The well-known ridge regression algorithm has
74 been widely used to solve this problem [16]. Another commonly used technique is the boosting algorithm, which is a sparse
75 estimation technique belonging to the broad family of greedy additive estimators, and solves the TRF problem using coordinate
76 descent [14], [15], [31]. In brief, this algorithm starts from an all-zero TRF and incrementally adds small, fixed values to the TRF
77 to decrease the mean square error (MSE) at each iteration. The iterations are stopped when the MSE does not improve. A
78 dictionary of basis elements (e.g., Hamming windows) is used for the incremental additions to the TRF. Both ridge and boosting
79 can be used independently at each sensor to estimate TRFs for multi-channel data.

80

81 B. Proposed SP algorithm for TRF estimation

82 The SP algorithm searches for TRF components within predefined latency windows and directly estimates them. This is unlike
83 the ridge and boosting algorithms that do not place specific restrictions on the number or latencies of detected TRF components.
84 Assuming there are J components (e.g., $J = 3$ for M50, M100, M200 components), the TRF model is now given by a modified
85 version of (1).

$$\mathbf{y} = \sum_{j=1}^J a_j \mathbf{X} \mathbf{c}_j + \mathbf{n} \quad (3)$$

86 Where $a_j \in \mathbb{R}$ and $\mathbf{c}_j \in \mathbb{R}^K$ are the amplitude and waveform for the j^{th} component. The component waveforms \mathbf{c}_j are selected
87 according to the component latency τ_j from a basis dictionary (e.g., Hamming windows) that span the TRF lags (i.e., \mathbf{c}_j is
88 column number τ_j of the basis dictionary matrix). The SP algorithm directly estimates the amplitudes a_j and latencies τ_j . The
89 complete algorithm is given in Algorithm 1.

90

91

92

93

94

95

96

97

98

99

Algorithm 1: SP for TRF estimation

Inputs: Measured signal $\mathbf{y} \in \mathbb{R}^T$, predictor matrix $\mathbf{X} \in \mathbb{R}^{T \times K}$, number of components J and corresponding latency windows W_j

- 1: Initialize the set of TRF components to the empty set; $\mathcal{C}^0 = \emptyset$.
- 2: Set the residual to the measured signal $\mathbf{r}^0 = \mathbf{y}$
- 3: **repeat** for $l = 1, 2, \dots$
- 4: **repeat** for $j = 1, \dots, J$
- 5: Find the best component latency
 $\mathbf{c}_j^* = \operatorname{argmax}_{\tau \in W_j} |\langle \mathbf{r}^l, \mathbf{X}\mathbf{c}_\tau \rangle|$
 where \mathbf{c}_τ is the basis component with latency τ
- 6: Add the J new components to the set $\tilde{\mathcal{C}} = \mathcal{C}^{l-1} \cup \{\mathbf{c}_j^*\}$
- 7: Estimate amplitudes $\tilde{\mathbf{a}} = (\mathbf{A}^T \mathbf{A})^{-1} \mathbf{A}^T \mathbf{y}$
 where \mathbf{A} has columns $\{\mathbf{X}\mathbf{c} \mid \mathbf{c} \in \tilde{\mathcal{C}}\}$
- 8: Update the component set
 $\mathcal{C}^l = \{J \text{ components with the largest amplitudes for each } W_j\}$
- 9: Re-estimate amplitudes $\mathbf{a}^l = (\mathbf{B}^T \mathbf{B})^{-1} \mathbf{B}^T \mathbf{y}$
 where \mathbf{B} has columns $\{\mathbf{X}\mathbf{c} \mid \mathbf{c} \in \mathcal{C}^l\}$
- 10: Calculate the new residual $\mathbf{r}^l = \mathbf{y} - \mathbf{B}\mathbf{a}^l$
- 11: If $\|\mathbf{r}^l\| > \|\mathbf{r}^{l-1}\|$ stop iterations and set $\mathcal{C}^l = \mathcal{C}^{l-1}$ & $\mathbf{a}^l = \mathbf{a}^{l-1}$

Output: amplitudes $\mathbf{a}^l = [a_1, \dots, a_J]$, components $\mathbf{c}_j \in \mathcal{C}^l$ and TRF $\boldsymbol{\beta} = \sum_{j=1}^J a_j \mathbf{c}_j$.

100

101 The SP algorithm estimates TRFs composed of only the required number of components, and can also be applied
 102 independently at each sensor for multi-channel TRFs.

103 *C. Proposed EM-SP algorithm for TRF Estimation*

104 The EM-SP algorithm is an extension of the SP algorithm for multidimensional TRFs. In addition to directly estimating
 105 amplitudes and latencies, this algorithm also directly estimates sensor topographies or source distributions for multi-channel
 106 TRFs. This algorithm uses EM to iteratively estimate component topographies in the E-step, and latencies using SP in the M-
 107 step. Given a predefined number of components and corresponding latency windows, the EM-SP multi-channel TRF model is
 108 given by a modified version of (3).

$$\mathbf{Y} = \sum_j \mathbf{z}_j (\mathbf{X}\mathbf{c}_j)^T + \mathbf{N} \quad (4)$$

109 Where $\mathbf{Y} \in \mathbb{R}^{M \times T}$ is the measured data over M sensors and T time points, $\mathbf{z}_j \in \mathbb{R}^M$ is the spatial topography of the j^{th} component,
 110 $\mathbf{c}_j \in \mathbb{R}^K$ is the temporal waveform of the j^{th} component, $\mathbf{X} \in \mathbb{R}^{T \times K}$ is the predictor matrix, and $\mathbf{N} \in \mathbb{R}^{M \times T}$ is the measurement noise.
 111 The component latency is given by τ_j and is related to (4) by the fact that \mathbf{c}_j corresponds to column number τ_j in the TRF basis
 112 dictionary matrix. We assume the following priors,

$$\begin{aligned} \mathbf{z}_j &\sim \mathcal{N}(\boldsymbol{\mu}, \mathbf{R}) \\ \mathbf{N} &\sim \mathcal{N}(\mathbf{0}, \mathbf{I}_{T \times T} \otimes \boldsymbol{\Lambda}) \end{aligned} \quad (5)$$

113 Where the temporal noise covariance is assumed to be the identity matrix and the spatial noise covariance is given by
 114 $\boldsymbol{\Lambda} \in \mathbb{R}^{M \times M}$. For the EM algorithm, we consider the spatial topographies $\mathcal{Z} = \{\mathbf{z}_j\}$ as the ‘hidden’ variables. The remaining

115 parameters that need to be estimated are $\Theta = \{\boldsymbol{\mu}, \mathbf{R}, \boldsymbol{\Lambda}, \tau_j\}$. Detailed derivations of the algorithm are provided in supplementary
 116 materials. Here, we summarize the main steps of the algorithm.

117 The Q-function is given by taking the expectation over the posterior probability $p(\mathcal{Z}|\mathbf{Y}, \Theta)$.

$$Q(\Theta|\theta^{(t)}) = \frac{T}{2} \log|\boldsymbol{\Lambda}^{-1}| + \frac{I}{2} \log|\mathbf{R}^{-1}| - \frac{1}{2} \text{tr}[\mathbf{Y}^T \boldsymbol{\Lambda}^{-1} \mathbf{Y}] + \text{tr}[\mathbf{Y}^T \boldsymbol{\Lambda}^{-1} (\sum_j \mathbf{E}[\mathbf{z}_j] \mathbf{x}_j^T)] - \frac{1}{2} \text{tr}[\sum_i \sum_j \mathbf{x}_j^T \mathbf{x}_i \mathbf{E}[\mathbf{z}_j \mathbf{z}_i^T] \boldsymbol{\Lambda}^{-1}] \\ - \frac{1}{2} \sum_j \text{tr}(\mathbf{E}[\mathbf{z}_j \mathbf{z}_j^T] \mathbf{R}^{-1}) - 2\boldsymbol{\mu}^T \mathbf{R}^{-1} \mathbf{E}[\mathbf{z}_j] + \boldsymbol{\mu}^T \mathbf{R}^{-1} \boldsymbol{\mu} \quad (6)$$

118 In the Expectation step, the posterior means of the spatial topographies are estimated.

$$\bar{\mathbf{z}}_j = (\mathbf{x}_j^T \mathbf{x}_j \boldsymbol{\Lambda}^{-1} + \mathbf{R}^{-1})^{-1} (\boldsymbol{\Lambda}^{-1} (\mathbf{Y} - \sum_{i \neq j} \bar{\mathbf{z}}_i \mathbf{x}_i^T) \mathbf{x}_j + \mathbf{R}^{-1} \boldsymbol{\mu}) \quad (7)$$

119 For the Maximization step, we use the Conditional Maximization method [32] whereby we sequentially maximize over each
 120 one of the parameters $\Theta = \{\boldsymbol{\mu}, \mathbf{R}, \boldsymbol{\Lambda}, \tau_j\}$, while holding the others fixed at their previous values.

$$\boldsymbol{\mu} = \frac{1}{J} \sum \bar{\mathbf{z}}_j \quad (8)$$

$$\mathbf{R} = \frac{1}{JM} \sum (\mathbf{S}_j + \bar{\mathbf{z}}_j \bar{\mathbf{z}}_j^T - \boldsymbol{\mu} \bar{\mathbf{z}}_j^T - \bar{\mathbf{z}}_j \boldsymbol{\mu}^T + \boldsymbol{\mu} \boldsymbol{\mu}^T) \quad (9)$$

$$\boldsymbol{\Lambda} = \frac{1}{T} \mathbf{Y} \mathbf{Y}^T - \mathbf{Y} (\sum \bar{\mathbf{z}}_j \mathbf{x}_j^T)^T - (\sum \bar{\mathbf{z}}_j \mathbf{x}_j^T) \mathbf{Y}^T \\ + \sum_j (\mathbf{x}_j^T \mathbf{x}_j (\mathbf{S}_j + \bar{\mathbf{z}}_j \bar{\mathbf{z}}_j^T)^T + \sum_{i \neq j} \mathbf{x}_j^T \mathbf{x}_i \bar{\mathbf{z}}_i \bar{\mathbf{z}}_i^T) \quad (10)$$

121 The latencies τ_j can be estimated in a similar manner to the single channel SP algorithm using a linear search to maximize
 122 $\text{tr} \left[(\mathbf{Y} - \sum_{i \neq j} \bar{\mathbf{z}}_i \mathbf{x}_i^T)^T \boldsymbol{\Lambda}^{-1} \bar{\mathbf{z}}_j \mathbf{x}_j^T \right]$ over the component basis. The complete EM-SP algorithm is provided below.

123

124

125

126

127

128

129

130

131

132

133

134

135

136

137

Algorithm 2: EM-SP

Inputs: Multi-channel data $\mathbf{Y} \in \mathbb{R}^{M \times T}$, $\mathbf{X} \in \mathbb{R}^{T \times K}$, the number of components J and latency windows W_j

- 1: Initialize parameters $\bar{\mathbf{z}}_j$ and $\theta^0 = \{\tau_j^0, \boldsymbol{\mu}^0, \mathbf{R}^0, \boldsymbol{\Lambda}^0\}$.
 - 2: **repeat** for $t = 1, 2, \dots$
 - 3: E-step: Estimate the spatial topographies $\bar{\mathbf{z}}_j$ using (7)
 - 4: CM-steps: Estimate parameters $\boldsymbol{\mu}^t, \mathbf{R}^t, \boldsymbol{\Lambda}^t$ using (8)-(10)
CM-step: Estimate the latencies τ_j^t using SP as shown below
 - 5: Initialize residual $\mathbf{Y}_R^0 = \mathbf{Y}$ and component set $\mathcal{C}^0 = \emptyset$
 - 6: Normalize the spatial topographies $\bar{\mathbf{z}}_j = \bar{\mathbf{z}}_j / \max(|\bar{\mathbf{z}}_j|)$
 - 7: **repeat** for iterations $l = 1, 2, \dots$
 - 8: **repeat** for components $j = 1, \dots, J$
 - 9: Find the best component latency

$$\mathbf{c}_j^* = \operatorname{argmax}_{\tau \in W_j} \operatorname{tr}((\mathbf{Y}_R^{l-1})^T \boldsymbol{\Lambda}^{-1} \bar{\mathbf{z}}_j (\mathbf{X} \mathbf{c}_\tau)^T)$$

where \mathbf{c}_τ is the basis component with latency τ
 - 10: Add the J new components to the set $\tilde{\mathcal{C}} = \mathcal{C}^{l-1} \cup \{\mathbf{c}_j^*\}$
 - 11: Estimate amplitudes $\tilde{\mathbf{a}} = (\mathbf{A}^T \mathbf{A})^{-1} \mathbf{A}^T \mathbf{y}$

where $\mathbf{y} = \operatorname{vec}(\boldsymbol{\Lambda}^{-\frac{1}{2}} \mathbf{Y})$ is the vectorized whitened data
and \mathbf{A} has columns $\{\operatorname{vec}(\boldsymbol{\Lambda}^{-\frac{1}{2}} \bar{\mathbf{z}}_j (\mathbf{X} \mathbf{c}_j)^T) \mid \mathbf{c}_j \in \tilde{\mathcal{C}}\}$
 - 12: Update $\mathcal{C}^l = \{J \text{ components with the largest amplitudes for each } W_j\}$
 - 13: Re-estimate amplitudes $\mathbf{a}^l = (\mathbf{B}^T \mathbf{B})^{-1} \mathbf{B}^T \mathbf{y}$

where \mathbf{B} has columns $\{\operatorname{vec}(\boldsymbol{\Lambda}^{-\frac{1}{2}} \bar{\mathbf{z}}_j (\mathbf{X} \mathbf{c}_j)^T) \mid \mathbf{c}_j \in \mathcal{C}^l\}$
 - 14: Calculate the new residual $\mathbf{Y}_R^l = \mathbf{Y} - \sum_j a_j \bar{\mathbf{z}}_j (\mathbf{X} \mathbf{c}_j)^T$

where a_j are the values in \mathbf{a}^l
 - 15: If $\|\mathbf{Y}_R^l\| > \|\mathbf{Y}_R^{l-1}\|$ stop iterations, let $\mathcal{C}^l = \mathcal{C}^{l-1}$ & $\mathbf{a}^l = \mathbf{a}^{l-1}$
 - 16: Update the spatial topographies $\bar{\mathbf{z}}_j = a_j \bar{\mathbf{z}}_j$
- Output:** The estimated TRF $\boldsymbol{\beta} = \sum_{j=1}^J \bar{\mathbf{z}}_j \mathbf{c}_j^T$, spatial topographies $\bar{\mathbf{z}}_j$, and components \mathbf{c}_j with latencies τ_j and amplitudes $a_j = \max(|\bar{\mathbf{z}}_j|)$.
-

138

139 All four algorithms can also be used to simultaneously fit TRFs to multiple predictors (e.g., foreground and background
 140 envelopes) by concatenating the P predictor matrices $X_p \in \mathbb{R}^{T \times K}$ along the columns, resulting in a new predictor matrix $X \in$
 141 $\mathbb{R}^{T \times KP}$. In this work, we jointly fit TRFs to two predictors (corresponding to foreground and background speech envelopes)
 142 using a concatenated predictor matrix.

143

144 D. Simulation Study

145 Simulations were constructed to match typical cocktail party speech experiments which have two simultaneous speech
 146 streams. Accordingly, the envelopes of two speech stimuli (foreground and background) were used as predictors. These
 147 envelopes were constructed by first passing the speech waveform through a gammatone filterbank with 256 frequency bands

148 between 20-4000 Hz, and the amplitude spectrogram was computed with an integration window of 10 ms. The resulting
149 spectrogram was averaged across frequency bands, downsampled to 1000 Hz, and then band-passed at 1-10 Hz using a
150 symmetric linear phase FIR filter with order 3301 and cutoffs 0.5 Hz and 11.25 Hz. Finally, the envelopes were downsampled to
151 100 Hz for all further analysis. These envelopes were repeated three times, in line with experiments having multiple trials of
152 repeated stimuli to extract consistent responses using spatial filters such as Denoising Source Separation (DSS [33]; details given
153 below). Each predictor was convolved with its own ground truth simulated TRF and the responses were summed together to
154 form one-dimensional responses at 100 Hz sampling rate for 30 pseudo-subjects comparable to a single-sensor M/EEG response
155 or the first auditory response component after DSS.

156 For each simulated subject, the ground truth simulated TRF was formed by placing Hamming windows of 50 ms width with
157 peaks in the latency ranges 30-80 ms, 90-170 ms and 190-250 ms corresponding to typical latencies of the M50, M100 and
158 M200 components. The M100 component was given a negative sign, and the components were scaled and shifted according to
159 randomized subject specific amplitudes and latencies. These amplitudes and latencies were later used as the ground truth for
160 performance evaluation.

161 Realistic noise was added to the simulated responses using the first DSS component of real MEG data collected from 30
162 subjects listening to speech (previously published [34], [35]). DSS creates a series of spatial filters, where the DSS component
163 generated by the first of these filters corresponds to activity that is most consistent across repeated stimulus presentations (see
164 [33] for details on DSS). Therefore, for this speech experiment, the first DSS component is dominated by auditory activity and
165 displays a typical auditory response sensor topography. This component was then phase scrambled, preserving the spectral
166 properties of MEG signals, to simulate noise added to the simulated response, at SNRs of -15, -20, -25 and -30 dB (SNRs
167 selected to result in realistic TRF model correlation values).

168 The multi-channel simulation followed the same method for 157 simulated sensor signals, but in addition also used ground
169 truth sensor topographies for each TRF component. These topographies were constructed from the TRF component topographies
170 of a real subject with typical auditory TRF components, with the addition of Gaussian noise to simulate individual variability.
171 Real multi-channel MEG data was again phase scrambled and added as noise on a per channel basis using the method described
172 above, at SNRs of -20, -25, -30 and -35 dB (lower SNRs were used because unprocessed multi-channel data is typically noisier
173 than the extracted auditory component).

174 The DSS algorithm was also applied to the simulated multi-channel data and corresponding TRFs were calculated for the first
175 6 DSS components. These DSS TRFs were projected back into sensor space for subsequent analysis and for computing
176 performance metrics.

177 The source space simulation was constructed using the Freesurfer ico-4 surface source space of the ‘fsaverage’ brain [36]. An
178 ROI in temporal lobe with 245 sources that included auditory cortex was used for this simulation (‘aparc’ labels
179 ‘transversetemporal’ and ‘superiortemporal’). The three TRF components were simulated using dipoles in Heschl’s gyrus,
180 Planum Temporale and Superior Temporal Gyrus in both hemispheres. These dipoles were projected onto the sensors using
181 forward models from real data and back projected back onto source space with Minimum Norm Estimation (MNE) [37] using
182 Eelbrain [14], [38] and MNE-Python softwares [39] to simulate the source localization procedure. The back-projected source
183 distributions of these simulated TRF components were also used as the ground truth for subsequent performance comparisons.
184 The TRFs were then convolved with the predictors to form the responses at each of the 245 sources. Real MEG data was phase
185 scrambled and added as noise to the response at each source at SNRs of -15, -20, -25 and -30 dB following the same procedure
186 as above.

187

188 *E. Experimental Dataset*

189 MEG data collected in a prior study [34], [35] was used for evaluating the performance of the algorithms on real data. The
190 study was approved by the IRB of the University of Maryland and all participants provided written informed consent prior to the
191 start of the experiment. The dataset consisted of MEG data collected from 40 subjects while they listened to speech from the
192 narration of an audiobook. Subjects listened to two speakers simultaneously in a cocktail party experiment, but were asked to
193 attend to only one speaker. The data was from the condition where the foreground speaker was 3 dB louder than the background
194 speaker. TRFs were estimated for the foreground and background envelopes. Whole head sensor space TRFs (157 sensors) were
195 computed for each algorithm on three minutes of data. Additionally, TRFs were also computed for the first 6 DSS components.
196 Finally, the MEG responses of this dataset were source localized using MNE and source space TRFs were also computed.

197

198 *F. Algorithm Implementation*

199 The algorithms were implemented in Python (version 3.9.6) using SciPy (version 1.8.0) [40], and Eelbrain (version 0.36.1).
200 The code is available online at <URLs available upon acceptance>. A basis dictionary with Hamming windows of width 50 ms
201 was used for boosting, SP and EM-SP. The component latency windows for the SP and EM-SP algorithms were 30-80 ms, 90-
202 170 ms and 190-250 ms. To avoid instability and convergence issues, the spatial covariance \mathbf{R} for the EM-SP algorithm was
203 assumed to be the identity matrix. The EM-SP was initialized using the extracted components from the SP algorithm applied at
204 each sensor/source independently.

205 A nested 4-fold cross validation procedure was followed for all algorithms to allow for unbiased comparison. The data was
206 divided into 4 splits, with 1 for testing, 1 for validation and 2 for training. The validation and training splits were permuted for
207 each test split in a nested fashion. The training data was used to optimize the ridge TRF over several regularization parameters
208 (steps of $2^0, 2^1, \dots, 2^{16}$) based on the model fit on the validation data. The boosting TRF was fit on the training data, and the
209 validation data was used to check for convergence and terminate the algorithm. The SP and EM-SP TRFs were fit on the training
210 data, and the model fit on the validation data was used to terminate the EM iterations. Finally, the overall model fit metric was
211 calculated by convolving the average TRF over all training splits with the appropriate test predictor and computing the Pearson
212 correlation between this predicted signal and the actual test signal.

213 *G. Performance Metrics*

214 The model fit was calculated as the Pearson correlation between the estimated and the predicted response (averaged over
215 channels for multidimensional cases). A null model was constructed by fitting TRFs using circularly time-shifted predictors
216 (shifts of 15 s) and the correlation of this null model was subtracted from the true model. This bias corrected model fit is reported
217 for both simulations and real data.

218 In addition to model fit, several other metrics of TRF component estimation were also calculated for the simulations (but not
219 for real data, since the ground truth components were unknown). TRF components were automatically detected as the peaks of
220 the r.m.s of the TRF across channels in the appropriate latency windows (30-80 ms, 90-170 ms, 190-250 ms) and the following
221 metrics were used; 1) Pearson correlation between the estimated and ground truth TRF, 2) Absolute error of individual
222 component latency estimates 3) Absolute error of individual component amplitude estimates (estimated vs, ground truth), 4)
223 Spurious TRF activity given by the % r.m.s. power in the estimated TRF after 300 ms (note that there is no activity in the ground
224 truth TRF after 300 ms), 5) Number of missing components 6) Sensor/source topography estimation error using the angle
225 between the estimated topography vector and the ground truth topography vector. These metrics were averaged over channels,
226 predictors, and components.

227

III. RESULTS

228 A. Simulation: Single-Channel TRFs

229 Single-channel TRFs were simulated, and the ridge, boosting, and SP algorithms were compared in terms of several
 230 performance metrics. The estimated TRFs for a representative subject are shown in Fig. 1. The conventional measure for
 231 evaluating the performance of TRF models is the correlation between the actual and the predicted responses. In this work we
 232 used a nested cross-validation procedure for all algorithms to reduce overfitting and a null model based on shifted predictors for
 233 bias correction. However, correlation between the actual and the predicted responses may not always be an appropriate measure
 234 of TRF component estimation, since it depends on a variety of factors including SNR and predictor characteristics. This metric
 235 may also not appropriately penalize latency errors or spurious activity in the TRF. Hence, we used several other metrics,
 236 including component latency and amplitude errors, to compare these algorithms in terms of TRF component estimation (see right
 237 column of Fig. 1).

238 The SP algorithm performed the best in most measures, while ridge and boosting performed comparably. Spurious peaks after
 239 300 ms (when there was no activity in the ground truth TRF) could lead to difficulties in interpretation and to false positives
 240 when detecting TRF components in real data. Conversely, missing components (false negatives) could also lead to improper
 241 interpretation of TRFs. Ridge had more spurious activity than boosting but was also able to detect more components than
 242 boosting.

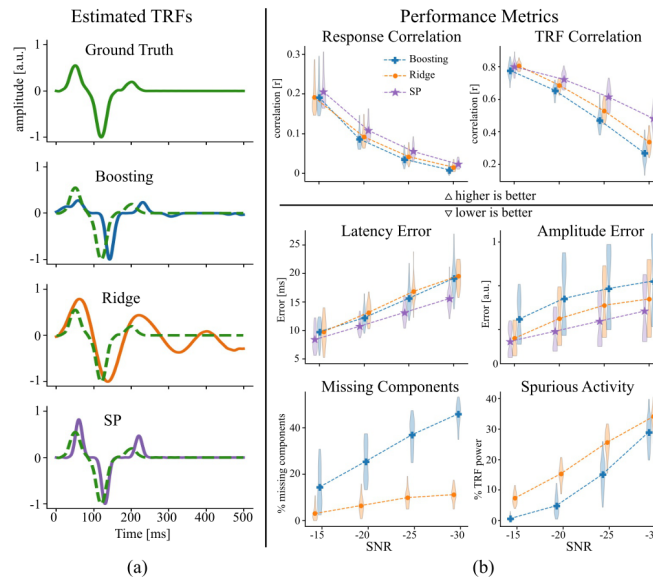


Fig. 1. Performance comparison for single-channel simulations. (a) The fitted TRFs for a representative subject. The ground truth TRF is shown as a dotted green line over the estimated TRFs. (b) Algorithm comparison using the performance metrics. Violin plots over simulated subjects are shown, with the symbols indicating the mean. Within each SNR condition, the algorithms are plotted in ascending order of their means from left to right. SP does not have spurious activity after 300 ms or missing components by design and is not shown for the bottom two subplots. Boosting seems to miss some components, while ridge has more spurious activity. Ridge and boosting are comparable for most measures, while SP seems to outperform the others in higher SNR cases.

243

244 B. Simulation: Multi-channel TRFs

245 Sensor space TRFs were simulated using realistic sensor topographies for TRF components, and the performance of each
 246 algorithm was compared (see Fig. 2). TRFs were estimated independently at each sensor for the boosting, ridge and SP
 247 algorithms, while the EM-SP algorithm directly estimated multi-channel component topographies. The EM-SP algorithm
 248 performed the best in most measures, while ridge and boosting performed comparably. The sensor topographies estimated by
 249 boosting and SP are worse than those estimated by ridge and EM-SP, which is to be expected given that the former are sparse
 250 algorithms that are fit at each sensor independently. Interestingly, the missing components are similar for both ridge and

251 boosting, unlike in the single-channel case. If boosting is able to correctly estimate components even for only a few channels,
 252 sparsity (in time) can then preserve the presence of the component peak when the r.m.s of the TRF is taken across channels. This
 253 improvement in component detection for boosting is also seen for the DSS and source space TRFs reported below.

254

255

256 *C. Simulation: Denoised TRFs using DSS*

257 The DSS algorithm was applied to the simulated sensor space responses to extract spatial filters corresponding to auditory
 258 response components. The algorithms were fit on the first 6 DSS components, and the resulting TRFs were projected back onto
 259 the sensor space for performance evaluation. Model fit response correlations increased greatly over the sensor space TRFs in all
 260 cases (see Fig. 3). Ridge, boosting and EM-SP had comparable results. Interestingly, EM-SP did not have a significant advantage
 261 over the other algorithms, indicating that the established algorithms are just as suitable for low dimensional, denoised data.

262

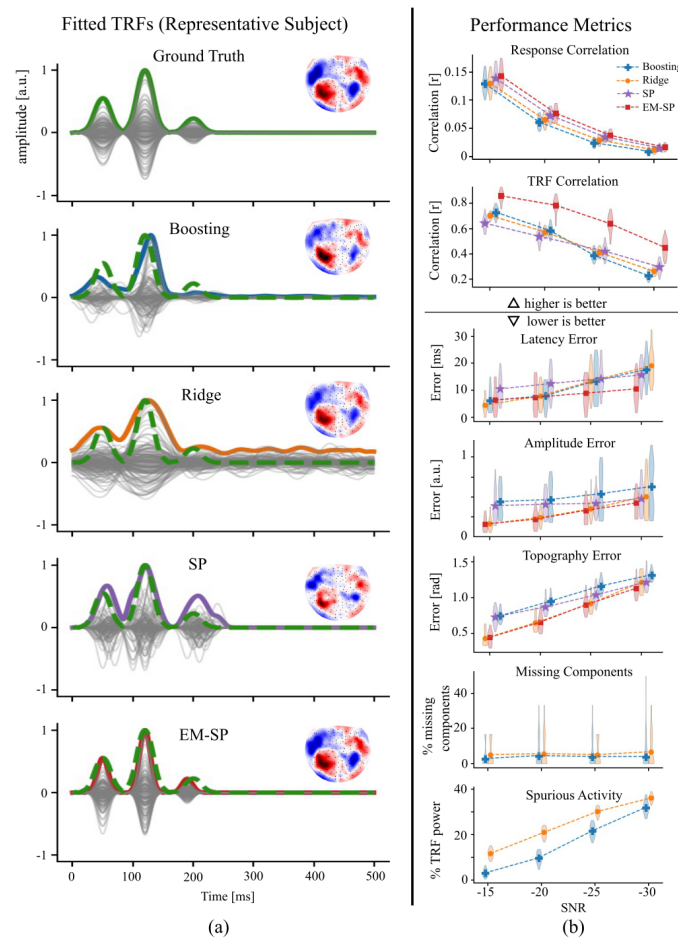


Fig. 2. Performance comparison for multi-channel simulations. (a) The fitted TRFs for a representative subject. The TRF at each sensor is plotted in gray, while the ℓ_2 -norm over sensors is plotted as a colored thick line. The ℓ_2 -norm of the ground truth TRF is shown as a dotted green line over the estimated TRFs. The sensor topography at the largest peak near 100 ms is shown as an inset. (b) Algorithm comparison using the performance metrics. Since there is no activity after 300 ms in the SP and EM-SP TRFs by design, they are not plotted in the spurious activity subplot. EM-SP outperforms the others in most measures. Although all methods find similar components, the sensor topographies for boosting and SP are worse than the others, perhaps because they are sparse estimation techniques.

263

264

265 *D. Simulation: Source Localized TRFs*

266 Source space simulations were constructed with dipoles in auditory areas for each TRF component. These dipoles were
 267 projected onto sensor space using the forward model and source localized back to source space to simulate source localized
 268 MEG data. The algorithms were fit on these source localized signals and performance was compared using the same metrics (see
 269 Fig. 4). Results were similar to the sensor space simulation, with EM-SP outperforming the others, and ridge and boosting giving
 270 comparable results (with ridge typically performing marginally better than boosting for most measures except spurious activity).

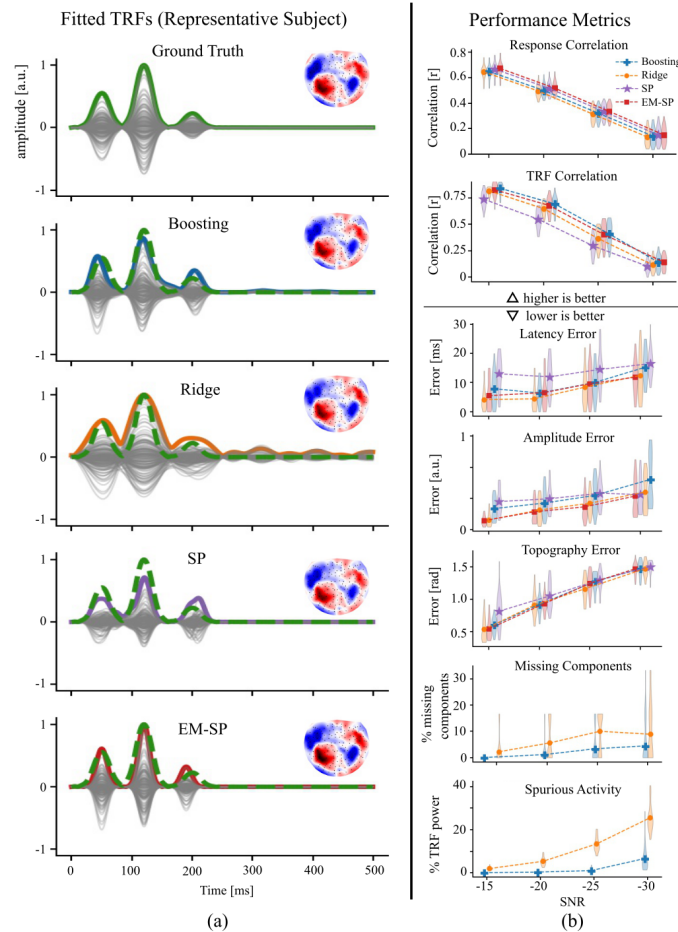


Fig. 3. Performance comparison after DSS denoising. (a). The fitted TRFs for a representative subject, similar to the previous figure. The TRFs were fit on the first 6 DSS components and then back-projected to sensor space. All the algorithms result in reasonable TRF components and sensor topographies. (b). Algorithm comparison using the performance metrics. All the algorithms except SP perform comparably, while the latter performs the worst in most cases.

271
 272 Overall, the simulation results indicate that both boosting and ridge are comparable, with ridge typically performing slightly
 273 better. Interestingly, SP outperformed ridge and boosting in the high noise single-channel simulations, while EM-SP
 274 outperformed the others by a large margin in the multi-channel and source-localized simulations. It should be noted that the
 275 component windows used for the simulation were identical to the component windows provided a-priori to SP and EM-SP,
 276 which may explain their better performance. Therefore, SP and EM-SP may be suitable for estimating TRFs in high noise
 277 conditions, assuming that the appropriate latency windows can be determined a-priori. Ridge also had lower spatial error
 278 compared to boosting (sensor topography and source distribution errors), perhaps because a sparse estimation technique like
 279 boosting cannot capture smooth spatial patterns as well as ridge. Conversely, ridge had much larger amounts of spurious activity
 280 compared to boosting. However, after applying the DSS algorithm, ridge, boosting and EM-SP once again showed comparable
 281 performance, highlighting the importance of denoising methods when estimating TRFs from noisy multidimensional data.

283

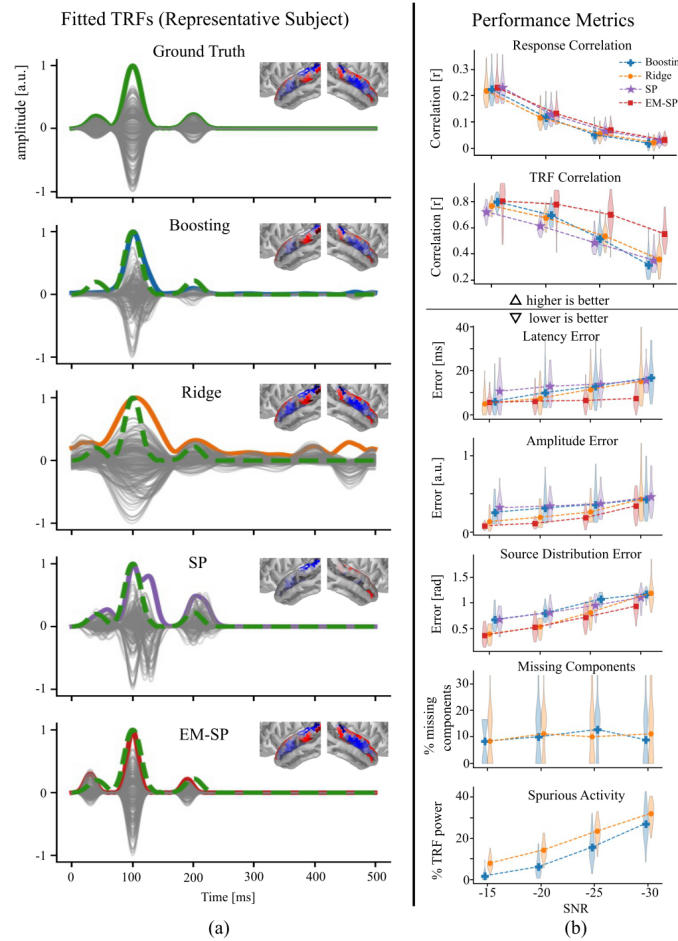


Fig. 4. Performance comparison for source space simulations. (a) The fitted TRFs for a representative subject are shown, similar to the previous figure. The source distributions in the temporal lobe ROI at the largest peak near 100 ms are shown as insets. Boosting and SP result in much sparser source distributions, and all the algorithms except SP perform comparably in estimating the TRF components, although the ridge TRF has a lot more activity that may make it difficult to interpret in realistic situations where the ground truth is unknown. (b). Algorithm comparison using the performance metrics, similar to those shown in the previous figure. EM-SP outperforms the others in most cases.

284

285

286 E. Performance on Real Data

287 The algorithms were compared on a real MEG dataset collected for a cocktail party experiment. Sensor space, DSS and source
 288 space TRFs are shown for a representative subject in Fig. 5. The only metric used was the correlation between the measured and
 289 predicted signals, since the other metrics cannot be calculated when the ground truth TRF components are unknown.
 290 Interestingly, boosting had significantly lower correlation accuracy compared to each of the three other algorithms for sensor and
 291 source space TRFs (paired samples permutation tests with Holm-Bonferroni correction; all comparisons with boosting resulted in
 292 $t_{39} > 4$, $p < 0.01$), but there were no significant differences in correlation accuracy between ridge, SP and EM-SP. However, it is
 293 unclear if correlation is the most suitable metric for evaluating the accuracy of estimating TRF components. The correlation
 294 values were distributed over a large range across subjects, possibly indicating a high degree of inter-subject variability in neural
 295 SNR for time-locked responses. Ridge resulted in smooth TRFs with several peaks and large amounts of non-zero activity which
 296 made them more difficult to interpret, especially for the sensor and source space TRFs. Boosting, though performing worse in
 297 terms of correlation, allowed for sparser TRFs with fewer peaks that were easier to interpret.

298

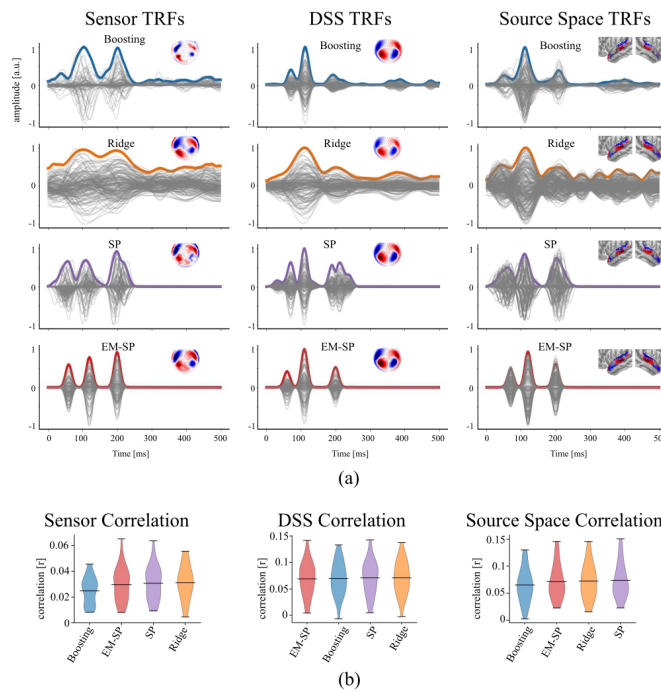


Fig. 5. Performance comparison on real MEG data. (a) The estimated sensor, DSS and source localized TRFs are shown for a representative subject. The sensor topographies and source distributions at the large peak near 100 ms are shown as insets. The sensor space EM-SP TRF has clear components and topographies, while the boosting TRF has overly sparse topographies and the ridge TRF has a lot of hard to interpret activity. Boosting, ridge and EM-SP show clear components and spatial patterns for the DSS and source localized TRFs. (b) Correlation between the measured and predicted signals is shown as a measure of model fit. Violin plots across subjects are shown for each algorithm in ascending order of their mean from left to right.

299

300

301

302

303

304

305

306

307

308

309

310

The two proposed algorithms were restricted to finding exactly three TRF components, assuming fixed component waveforms and latency windows. The fact that EM-SP may have performed worse than ridge for real data, even though it outperformed the others in the simulations, indicates that these assumptions may not be valid for all subjects. This could be due to a variety of reasons including missing components due to anatomical or functional differences, and large individual variability in TRF components latencies, waveforms, and peak widths. Indeed, a separate simulation analysis (not shown) with missing components and mismatched latency windows resulted in similar performance for EM-SP, with it no longer outperforming ridge and boosting. In any case, conventional post-hoc analysis of TRF components estimated using established algorithms is also typically performed under similar assumptions to those used for EM-SP (i.e., detecting TRF peaks using similar latency windows). However, even with these constraints, EM-SP was often able to recover TRF components and spatial patterns comparable to ridge.

311

IV. CONCLUSION

312

313

314

315

316

317

318

TRFs provide a significant advancement over ERPs, allowing for experiments with more naturalistic speech paradigms. Detecting robust TRF components is essential for reliable single-subject investigations that could inform diagnosis and treatment of hearing disabilities and lead to improved biomedical applications like smart hearing aids.

We compared TRF algorithms using both model fit and component estimation accuracy. Simulations indicate that boosting and ridge are comparable for most cases. Interestingly, ridge had better model fits on real data. However, in general, ridge TRFs displayed more spurious activity, while boosting TRF peaks were more interpretable. Therefore, ridge may be suitable for studies focused on prediction accuracy, while boosting may be appropriate for detecting easily identifiable TRF components. We

319 restricted our analysis of established methods to these two algorithms that are the most widely used. Other variations on
320 regularized regression, such as Lasso and Elastic Net, may provide improvements in TRF estimation [12].

321 SP and EM-SP performed exceptionally in simulations, but not on real data, possibly due to invalid assumptions. The a-priori
322 parameters may need to be tuned for each predictor type or experiment, or even for each subject

323 Modern TRF analyses involve multiple types of predictors [42] (e.g., envelopes, phoneme onsets, multiple frequency bands
324 for spectrotemporal TRFs). Boosting and banded ridge regression may be suitable for these studies [10], [13], [43], [44]. The
325 component characteristics of TRFs to these higher-level predictors must be determined before SP and EM-SP can be applied.
326 Additionally, early low-level responses could impact TRFs to high-level predictors, and sparse algorithms with fewer false
327 positives (but more false negatives) may be more conservative.

328 In conclusion, our results indicate that SP and EM-SP may only perform well under realistic assumptions, while ridge and
329 boosting perform comparably in most cases, with ridge typically having higher prediction accuracies, but also more spurious
330 activity.

331 REFERENCES

- 332 [1] T. Picton, "Hearing in Time: Evoked Potential Studies of Temporal Processing," *Ear and Hearing*, vol. 34, no. 4, pp. 385–401, 2013, doi:
333 10.1097/AUD.0b013e31827ada02.
- 334 [2] T. W. Picton, S. A. Hillyard, H. I. Krausz, and R. Galambos, "Human auditory evoked potentials. I: Evaluation of components," *Electroencephalography*
335 *and Clinical Neurophysiology*, vol. 36, pp. 179–190, Jan. 1974, doi: 10.1016/0013-4694(74)90155-2.
- 336 [3] N. Ding and J. Z. Simon, "Emergence of neural encoding of auditory objects while listening to competing speakers," *PNAS*, vol. 109, no. 29, pp. 11854–
337 11859, Jul. 2012, doi: 10.1073/pnas.1205381109.
- 338 [4] E. C. Lalor and J. J. Foxe, "Neural responses to uninterrupted natural speech can be extracted with precise temporal resolution," *European Journal of*
339 *Neuroscience*, vol. 31, no. 1, pp. 189–193, 2010, doi: 10.1111/j.1460-9568.2009.07055.x.
- 340 [5] S. Akram, J. Z. Simon, and B. Babadi, "Dynamic Estimation of the Auditory Temporal Response Function From MEG in Competing-Speaker
341 Environments," *IEEE Transactions on Biomedical Engineering*, vol. 64, no. 8, pp. 1896–1905, Aug. 2017, doi: 10.1109/TBME.2016.2628884.
- 342 [6] S. Geirnaert *et al.*, "Electroencephalography-Based Auditory Attention Decoding: Toward Neurosteered Hearing Devices," *IEEE Signal Processing*
343 *Magazine*, vol. 38, no. 4, pp. 89–102, Jul. 2021, doi: 10.1109/MSP.2021.3075932.
- 344 [7] C. Brodbeck, A. Jiao, L. E. Hong, and J. Z. Simon, "Neural speech restoration at the cocktail party: Auditory cortex recovers masked speech of both
345 attended and ignored speakers," *PLOS Biology*, vol. 18, no. 10, p. e3000883, Oct. 2020, doi: 10.1371/journal.pbio.3000883.
- 346 [8] C. Brodbeck, A. Presacco, and J. Z. Simon, "Neural source dynamics of brain responses to continuous stimuli: Speech processing from acoustics to
347 comprehension," *NeuroImage*, vol. 172, pp. 162–174, May 2018, doi: 10.1016/j.neuroimage.2018.01.042.
- 348 [9] M. P. Broderick, A. J. Anderson, G. M. Di Liberto, M. J. Crosse, and E. C. Lalor, "Electrophysiological Correlates of Semantic Dissimilarity Reflect the
349 Comprehension of Natural, Narrative Speech," *Current Biology*, vol. 28, no. 5, pp. 803–809.e3, Mar. 2018, doi: 10.1016/j.cub.2018.01.080.
- 350 [10] C. Brodbeck, L. E. Hong, and J. Z. Simon, "Rapid Transformation from Auditory to Linguistic Representations of Continuous Speech," *Current Biology*,
351 vol. 28, no. 24, pp. 3976–3983.e5, Dec. 2018, doi: 10.1016/j.cub.2018.10.042.
- 352 [11] C. Brodbeck, A. Presacco, S. Anderson, and J. Z. Simon, "Over-Representation of Speech in Older Adults Originates from Early Response in Higher
353 Order Auditory Cortex," *Acta Acustica united with Acustica*, vol. 104, no. 5, pp. 774–777, Sep. 2018, doi: 10.3813/AAA.919221.
- 354 [12] D. D. E. Wong, S. A. Fuglsang, J. Hjortkjær, E. Ceolini, M. Slaney, and A. de Cheveigné, "A Comparison of Regularization Methods in Forward and
355 Backward Models for Auditory Attention Decoding," *Front. Neurosci.*, vol. 12, 2018, doi: 10.3389/fnins.2018.00531.
- 356 [13] M. J. Crosse, N. J. Zuk, G. M. Di Liberto, A. R. Nidiffer, S. Molholm, and E. C. Lalor, "Linear Modeling of Neurophysiological Responses to Speech
357 and Other Continuous Stimuli: Methodological Considerations for Applied Research," *Front Neurosci*, vol. 15, p. 705621, Nov. 2021, doi:
358 10.3389/fnins.2021.705621.
- 359 [14] C. Brodbeck *et al.*, "Eelbrain: A Python toolkit for time-continuous analysis with temporal response functions," Aug. 2021. doi:
360 10.1101/2021.08.01.454687.
- 361 [15] S. V. David, N. Mesgarani, and S. A. Shamma, "Estimating sparse spectro-temporal receptive fields with natural stimuli," *Network*, vol. 18, no. 3, pp.
362 191–212, Sep. 2007, doi: 10.1080/09548980701609235.
- 363 [16] M. J. Crosse, G. M. Di Liberto, A. Bednar, and E. C. Lalor, "The Multivariate Temporal Response Function (mTRF) Toolbox: A MATLAB Toolbox for
364 Relating Neural Signals to Continuous Stimuli," *Front. Hum. Neurosci.*, vol. 0, 2016, doi: 10.3389/fnhum.2016.00604.

- 365 [17] C. D. Woody, "Characterization of an adaptive filter for the analysis of variable latency neuroelectric signals," *Medical & Biological Engineering*, vol. 5,
366 no. 6, pp. 539–554, Nov. 1967, doi: 10.1007/BF02474247.
- 367 [18] T.-P. Jung, S. Makeig, M. Westerfield, J. Townsend, E. Courchesne, and T. J. Sejnowski, "Analyzing and Visualizing Single-Trial Event-Related
368 Potentials," in *Advances in Neural Information Processing Systems 11*, M. J. Kearns, S. A. Solla, and D. A. Cohn, Eds. MIT Press, 1999, pp. 118–124.
369 Accessed: Oct. 02, 2020. [Online]. Available: <http://papers.nips.cc/paper/1574-analyzing-and-visualizing-single-trial-event-related-potentials.pdf>
- 370 [19] S. Makeig *et al.*, "Dynamic Brain Sources of Visual Evoked Responses," *Science*, vol. 295, no. 5555, pp. 690–694, Jan. 2002, doi:
371 10.1126/science.1066168.
- 372 [20] R. Q. Quiroga and H. Garcia, "Single-trial event-related potentials with wavelet denoising," *Clinical Neurophysiology*, vol. 114, no. 2, pp. 376–390, Feb.
373 2003, doi: 10.1016/S1388-2457(02)00365-6.
- 374 [21] J. C. de Munck, F. Bijma, P. Gaura, C. A. Sieluzycycki, M. I. Branco, and R. M. Heethaar, "A maximum-likelihood estimator for trial-to-trial variations in
375 noisy MEG/EEG data sets," *IEEE Transactions on Biomedical Engineering*, vol. 51, no. 12, pp. 2123–2128, Dec. 2004, doi:
376 10.1109/TBME.2004.836515.
- 377 [22] P. Jaskowski and R. Verleger, "Amplitudes and latencies of single-trial ERP's estimated by a maximum-likelihood method," *IEEE Transactions on*
378 *Biomedical Engineering*, vol. 46, no. 8, pp. 987–993, Aug. 1999, doi: 10.1109/10.775409.
- 379 [23] L. Xu, P. Stoica, J. Li, S. L. Bressler, X. Shao, and M. Ding, "ASEO: A Method for the Simultaneous Estimation of Single-Trial Event-Related Potentials
380 and Ongoing Brain Activities," *IEEE Transactions on Biomedical Engineering*, vol. 56, no. 1, pp. 111–121, Jan. 2009, doi:
381 10.1109/TBME.2008.2008166.
- 382 [24] T. Limpiti, B. D. Van Veen, and R. T. Wakai, "A Spatiotemporal Framework for MEG/EEG Evoked Response Amplitude and Latency Variability
383 Estimation," *IEEE Transactions on Biomedical Engineering*, vol. 57, no. 3, pp. 616–625, Mar. 2010, doi: 10.1109/TBME.2009.2032533.
- 384 [25] C. Sieluzycycki, R. Konig, A. Matysiak, R. Kus, D. Ircha, and P. J. Durka, "Single-Trial Evoked Brain Responses Modeled by Multivariate Matching
385 Pursuit," *IEEE Transactions on Biomedical Engineering*, vol. 56, no. 1, pp. 74–82, Jan. 2009, doi: 10.1109/TBME.2008.2002151.
- 386 [26] H. R. Mohseni, F. Ghaderi, E. L. Wilding, and S. Sanei, "Variational Bayes for Spatiotemporal Identification of Event-Related Potential
387 Subcomponents," *IEEE Transactions on Biomedical Engineering*, vol. 57, no. 10, pp. 2413–2428, Oct. 2010, doi: 10.1109/TBME.2010.2050318.
- 388 [27] W. Wu, C. Wu, S. Gao, B. Liu, Y. Li, and X. Gao, "Bayesian estimation of ERP components from multicondition and multichannel EEG," *NeuroImage*,
389 vol. 88, pp. 319–339, Mar. 2014, doi: 10.1016/j.neuroimage.2013.11.028.
- 390 [28] W. Dai and O. Milenkovic, "Subspace Pursuit for Compressive Sensing Signal Reconstruction," *IEEE Transactions on Information Theory*, vol. 55, no.
391 5, pp. 2230–2249, May 2009, doi: 10.1109/TIT.2009.2016006.
- 392 [29] A. P. Dempster, N. M. Laird, and D. B. Rubin, "Maximum Likelihood from Incomplete Data Via the EM Algorithm," *Journal of the Royal Statistical*
393 *Society: Series B (Methodological)*, vol. 39, no. 1, pp. 1–22, 1977, doi: 10.1111/j.2517-6161.1977.tb01600.x.
- 394 [30] C. B. Do and S. Batzoglou, "What is the expectation maximization algorithm?," *Nat Biotechnol*, vol. 26, no. 8, pp. 897–899, Aug. 2008, doi:
395 10.1038/nbt1406.
- 396 [31] T. Zhang and B. Yu, "Boosting with early stopping: Convergence and consistency," *The Annals of Statistics*, vol. 33, no. 4, pp. 1538–1579, Aug. 2005,
397 doi: 10.1214/009053605000000255.
- 398 [32] X.-L. Meng and D. B. Rubin, "Maximum Likelihood Estimation via the ECM Algorithm: A General Framework," *Biometrika*, vol. 80, no. 2, pp. 267–
399 278, 1993, doi: 10.2307/2337198.
- 400 [33] A. de Cheveigné and J. Z. Simon, "Denoising based on spatial filtering," *J Neurosci Methods*, vol. 171, no. 2, pp. 331–339, Jun. 2008, doi:
401 10.1016/j.jneumeth.2008.03.015.
- 402 [34] A. Presacco, J. Z. Simon, and S. Anderson, "Evidence of degraded representation of speech in noise, in the aging midbrain and cortex," *J Neurophysiol*,
403 vol. 116, no. 5, pp. 2346–2355, Nov. 2016, doi: 10.1152/jn.00372.2016.
- 404 [35] A. Presacco, J. Z. Simon, and S. Anderson, "Effect of informational content of noise on speech representation in the aging midbrain and cortex," *Journal*
405 *of Neurophysiology*, vol. 116, no. 5, pp. 2356–2367, Nov. 2016, doi: 10.1152/jn.00373.2016.
- 406 [36] B. Fischl, "FreeSurfer," *NeuroImage*, vol. 62, no. 2, pp. 774–781, Aug. 2012, doi: 10.1016/j.neuroimage.2012.01.021.
- 407 [37] M. S. Hämäläinen and R. J. Ilmoniemi, "Interpreting magnetic fields of the brain: minimum norm estimates," *Med. Biol. Eng. Comput.*, vol. 32, no. 1, pp.
408 35–42, Jan. 1994, doi: 10.1007/BF02512476.
- 409 [38] C. Brodbeck, P. Das, J. P. Kulsingham, S. Reddigari, and T. L. Brooks, *Eelbrain 0.36*. Zenodo, 2021. doi: 10.5281/zenodo.5152554.
- 410 [39] A. Gramfort *et al.*, "MNE software for processing MEG and EEG data," *NeuroImage*, vol. 86, pp. 446–460, Feb. 2014, doi:
411 10.1016/j.neuroimage.2013.10.027.
- 412 [40] P. Virtanen *et al.*, "SciPy 1.0: fundamental algorithms for scientific computing in Python," *Nature Methods*, vol. 17, no. 3, Art. no. 3, Mar. 2020, doi:
413 10.1038/s41592-019-0686-2.

- 414 [41] C. Brodbeck and J. Z. Simon, “Continuous speech processing,” *Current Opinion in Physiology*, vol. 18, pp. 25–31, Dec. 2020, doi:
415 10.1016/j.cophys.2020.07.014.
- 416 [42] M. Gillis, J. Vanthornhout, J. Z. Simon, T. Francart, and C. Brodbeck, “Neural Markers of Speech Comprehension: Measuring EEG Tracking of
417 Linguistic Speech Representations, Controlling the Speech Acoustics,” *J. Neurosci.*, vol. 41, no. 50, pp. 10316–10329, Dec. 2021, doi:
418 10.1523/JNEUROSCI.0812-21.2021.
- 419 [43] J. P. Kulasingham, N. H. Joshi, M. Rezaeizadeh, and J. Z. Simon, “Cortical Processing of Arithmetic and Simple Sentences in an Auditory Attention
420 Task,” *J. Neurosci.*, vol. 41, no. 38, pp. 8023–8039, Sep. 2021, doi: 10.1523/JNEUROSCI.0269-21.2021.
- 421 [44] J. P. Kulasingham, C. Brodbeck, A. Presacco, S. E. Kuchinsky, S. Anderson, and J. Z. Simon, “High gamma cortical processing of continuous speech in
422 younger and older listeners,” *NeuroImage*, vol. 222, p. 117291, Nov. 2020, doi: 10.1016/j.neuroimage.2020.117291.
- 423
- 424