Title: BOLD cofluctuation 'events' are predicted from static functional connectivity
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ABSTRACT

Recent work identified single time points ("events") of high regional cofluctuation in functional Magnetic Resonance Imaging (fMRI) which contain more large-scale brain network information than other, low cofluctuation time points. This suggested that events might be a discrete, temporally sparse signal which drives functional connectivity (FC) over the timeseries. However, a different, not yet explored possibility is that network information differences between time points are driven by sampling variability on a constant, static, noisy signal. Using a combination of real and simulated data, we examined the relationship between cofluctuation and network structure and asked if this relationship was unique, or if it could arise from sampling variability alone. First, we show that events are not discrete – there is a gradually increasing relationship between network structure and cofluctuation; ~50% of samples show very strong network structure. Second, using simulations we show that this relationship is predicted from sampling variability on static FC. Finally, we show that randomly selected points can capture network structure about as well as events, largely because of their temporal spacing. Together, these results suggest that, while events exhibit particularly strong representations of static FC, there is little evidence that events are unique timepoints that drive FC structure. Instead, a parsimonious explanation for the data is that events arise from a single static, but noisy, FC structure.

KEYWORDS

Resting-state fMRI, cofluctuations, events, simulations, RSFC, networks

HIGHLIGHTS

- Past results suggested high cofluctuation BOLD "events" drive fMRI functional connectivity, FC
- Here, events were examined in both real fMRI data and a stationary null model to test this model
- In real data, >50% of BOLD timepoints show high modularity and similarity to time-averaged FC
- Stationary null models identified events with similar behavior to real data
- Events may not be a transient driver of static FC, but rather an expected outcome of it.

INTRODUCTION

The human brain is organized in large-scale systems, or 'networks,' with coordinated functions such as the visual network, somatomotor network, and default mode network. In humans, these networks can be identified by grouping regions of the brain that have highly correlated spontaneous BOLD fMRI signals - regions with high "functional connectivity (FC)" (Biswal et al., 1995; Power et al., 2011; Yeo et al., 2011). These FC networks have been shown to have a canonical spatial layout (most people have the same networks represented in the same locations), with stable patterns of individual variation (each person's network topography is slightly different from the canonical layout and consistent within themselves across time (Gordon et al., 2017; Gratton et al., 2018; Laumann et al., 2015; Seitzman et al., 2019). At both the individual and group level, functional network topology accurately predicts which regions of the brain will be activated during specific tasks (Braga et al., 2020; Gordon et al., 2017; Smith et al., 2009; Tavor et al., 2016) and variations in network topology are related to individual differences in behavior outside of the scanner (Bijsterbosch et al., 2018; Kong et al., 2019; Smith et al., 2015; van den Heuvel et al., 2009)

However, analysis of spontaneous fMRI data is not straightforward. Unlike in task-fMRI, there is no predefined temporal structure that can be used to separate relevant signals from artifactual signals. Instead, typical analyses of spontaneous (resting-state) fMRI remove physiological artifacts (motion, respiration, cardiac rhythms, etc.) and assume the residual signal is the neural signal of interest (Power et al., 2020). It is typically presumed that this signal is equally present at all moments and FC is calculated using all available data over long periods. However, recent work suggested that rather than being constantly present, FC information might be inordinately present at particular time points called "events" (Esfahlani et al., 2020). Esfahlani and colleagues found that "events," time points with the highest BOLD signal cofluctuation, reproduce static functional connectivity patterns better than the same number of "non-events," time points with the lowest BOLD signal cofluctuation, and require relatively few timepoints to reproduce them well. The authors concluded that rather than functional network structure being present at all timepoints, it is driven by events – a discrete and temporally sparse phenomena (Esfahlani et al., 2020).This idea has deep implications for the field: a thorough analysis of events across brain organizational levels (e.g., from systems to cellular recordings) could reveal information about the physiological mechanisms of FC and new analysis methods focused on events could improve the clinical utility of fMRI (Esfahlani et al., 2021; Greenwell et al., 2021).

But, there are alternative interpretations of these findings which have not yet been explored. First, it is possible that differences between "events" and "non-events" are driven by contamination in "non-events" (motion, respiration, etc.) rather than by a unique signal present during "events." Second, it has been shown that random sampling variability in BOLD data is high and alone can create the appearance of discrete states in stationary FC simulations (Hlinka & Hadrava, 2015; Laumann et al., 2017). This principle may apply here too – sampling variability could make a subset of single points look extreme, even if they are drawn from a continuous distribution around a static FC matrix (note that if this were the case, events methodology may still be a useful way to rapidly and accurately reproduce static FC structure, but this outcome would suggest that a deep focus on events physiology relative to other timepoints has less utility). In this paper, we ask (1) if events are unique points which drive FC, (2) if non-events are unique points with high contamination, or (3) if events and non-events are an expected consequence of static FC and sampling variability.

To answer these questions, we conduct a series of analyses on real and simulated data. First, we use real data from the Midnight Scan Club dataset to test how unique events and non-events are by examining whether their properties differ markedly from intermediate timepoints. Second, we create models of simulated static BOLD data to see if sampling variability on a

97 static signal is sufficient to explain event behavior. Finally, we examine why events are able to
98 recreate static FC structure with so few time points.
99
100 **MATERIALS AND METHODS**
101
102 ***Overview and Dataset***
103 The goal of this project was to investigate if high cofluctuation moments in resting state fMRI
104 BOLD signals are discrete events that drive functional connectivity. We used a combination of
105 real and simulated data for these analyses.
106
The publicly available Midnight Scan Club (MSC) dataset was used as our real sample dataset.
The MSC dataset contains fMRI data from 10 highly sampled individuals (5 females, ages 24-
34). The data for each subject was collected across 10 fMRI sessions within 7 weeks. Across
these sessions, the MSC dataset includes 5 hours of resting state fMRI; this resting-state data is
the focus of our analyses. One participant (MSC08) has been excluded from these analyses
because of head motion and drowsiness during rest. For single session-analysis and
simulations, sessions with less than 333 usable timepoints (6/90 sessions) were excluded. All
data collection was approved by the Washington University Internal Review Board and written
informed consent was received from all participants. The dataset and processing have been
previously described in detail (Gordon et al., 2017). A summary of relevant details is provided
below.
118
MRI Acquisition
MRI data were acquired on a Siemens 3T Magnetom Tim Trio with a 12-channel head coil. T1-
weighted (sagittal, 224 slices, 0.8 mm isotropic resolution, TE = 3.74ms, TR = 2.4s, TI = 1.0s,
flip angle = 8 degrees), T2-weighted (sagittal, 224 slices, 0.8 mm isotropic resolution, TE =
479ms, TR = 3.2s) and functional (gradient-echo EPI sequence, TE = 27ms, TR = 2.2 s, flip
angle = 90, voxels =isotropic 4mm^3, 36 axial slices) MRI images were collected. Thirty minutes
of resting-state fMRI were collected at the start of each session.
126
127 ***Preprocessing***
128 Data processing for the MSC dataset is explained in detail elsewhere (Gordon et al., 2017).
129 Relevant details for this project are shared below.
130
131 Structural MRI Processing: For each participant, T1 images were averaged together and used
132 to generate a cortical surface in Freesurfer (Dale et al., 1999). These surfaces were hand-edited
133 and registered into fs_LR_32k surface space (Glasser et al., 2013).
134
135 Functional MRI Processing: Slice time correction, motion correction, and intensity normalization
136 to mode 1000 were all completed in the volume. The functional data was then registered to the
137 T2 image (which was registered to the T1 image registered to template space), resampled to
138 3mm isotropic resolution and distortion corrected (Gordon et al., 2017). All alignments were
139 applied in a single step.
140
Functional Connectivity Processing: Described in detail elsewhere (Power et al., 2014),
preprocessing steps were taken to reduce the effect of artifacts on functional network analysis.
This included the regression of nuisance signals (white matter, ventricles, global signal, motion
and derivative and expansion terms), scrubbing of high motion frames (FD > 0.2 mm), and
bandpass filtering (0.009 Hz to 0.08 Hz). For two subjects (MSC03 and MSC10), motion
parameters were low pass filtered before censoring to address respiratory activity in the motion

traces (Fair et al., 2020; Gordon et al., 2017). Functional data was then registered to the surface
and spatially smoothed (FWHM = 6 mm, sigma = 2.55) (Marcus et al., 2011).
149
Network and region definition
All analyses were done on parcellated timeseries extracted using a group-level map of 333
cortical parcels (Gordon et al., 2016). These 333 parcels can be split into 12 functional systems:
somatomotor (SM), somatomotor lateral (SM-lat), visual (Vis), auditory (Aud), cingulo-opercular
(CO), salience (Sal), frontoparietal (FP), dorsal attention (DAN), ventral attention (VAN), default
mode (DMN), parietal memory (PMN), and retrosplenial (RSP). These systems are used to
group parcels in the visualization of FC matrices.
157
Comparisons between events and static functional connectivity in real data
Our first goal was to compare the network structure present in events, non-events, and
intermediate bins. We followed the approach used in Esfahlani et al., 2020, calculating the RSS
(root-sum-square) cofluctuation for each timepoint and binning timepoints by their RSS
cofluctuation value. We compared the network structure present in each bin by creating FC
matrices for each bin and calculating the similarity between bin FC and whole session FC and
the modularity of bin FC. These measures are defined below.
165
Cofluctuation Time Series and Events: The method for calculating cofluctuation and identifying
events has been fully described elsewhere (Esfahlani et al 2020). It was followed exactly and is
summarized here. The original fMRI BOLD timeseries was z-scored per parcel. For each edge
(a unique pair of parcels), the z-scored values at each timepoint were multiplied, resulting in an
edges X timepoints matrix. As described elsewhere, this timeseries (also called the edge-time-
series), represents the exact contribution of each timepoint to static FC (Esfahlani et al., 2020).
For each time point, the RSS (root-sum-square) across parcels was calculated, resulting a 1 X
timepoints matrix containing the RSS cofluctuation value at each timepoint. Timepoints were
binned based on RSS cofluctuation value in 5% bins, with the 5% of points with highest
cofluctuation in bin one, the next 5% of points in bin two and so on.
176
Functional Connectivity (FC): For each session and subject, functional connectivity matrices
were calculated using either the timepoints from the full session ('static' FC matrices) or from
the timepoints in each bin (cofluctuation bin FC matrices). In all cases, FC was calculated by the
product moment correlation between each pair of parcel timeseries, resulting in a 333X333
functional network matrix. Parcels were grouped by functional system for visualization. Edges
within the diagonal blocks represent within-system correlations, and edges in the off-diagonal
blocks represent between-system correlations.
184
185 _Similarity_: Similarity between each bin's FC and whole-session 'static' FC was calculated by
186 vectorizing both matrices and taking the correlation between them.
187
Modularity: Modularity was calculated for each bin as measure of network structure. Modularity
maximization is a strategy used to arrange nodes into communities in which there are more
edges within communities than expected by random chance. Each matrix was thresholded for
sparseness, keeping only the top 5% of weighted edges (5% edge density). Then, all remaining
edge weights were set to 1, making the graph unweighted. Newman's spectral optimization was
used to identify the optimal network structure. This structure was then quantified using
Newman's modularity statistic, Q, which measures the fraction of within-network edges minus
the expected value of within-network edges in a network with the same communities but random
connections (Newman & Girvan, 2004). Larger values of modularity reflect stronger community
structure than expected by chance.

198
199 ***Comparisons between events and static functional connectivity in simulated data***
200 Our second goal was to test whether the relationship between network structure and
201 cofluctuation found in real data could be explained by sampling variability in a stationary model.
202 To examine this, we created simulated data with the same dimensionality and static covariance
203 structure as BOLD data but sampled from a random Gaussian distribution.
204
Simulated BOLD Data: For each subject and session, data was sampled from a Gaussian
distribution in the dimensionality of the real data from that session. Separately, a static FC
matrix was calculated from the full 30 minutes of real data. The random timeseries were
projected on to the eigenvectors derived from the static FC matrix, resulting in data matched in
dimensionality and covariance structure with real BOLD data but stationary by construction. This
strategy is largely adapted from prior simulation work (Laumann et al., 2017). We then did the
same analysis in the simulation data as was described above for real data – calculating
cofluctuation, binning frames by cofluctuation, and comparing the network structure present in
each bin with two measures (similarity to static FC and modularity).
214
Simulated Toy Model: To aid in our second goal, we did a supplementary analysis investigating
the relationship between network structure and cofluctuation in a very simple non-BOLD-like
data set. The data set comprised of 4 nodes total – 2 anti-correlated networks with two nodes
each. Network A was defined by the simple sine(x) wave, and both network A nodes were given
that signal. Network B was defined by sine(x + π/2) and both network B nodes were given that
signal. Normally distributed random noise of half the magnitude as the real signal was added to
all four nodes. Then, cofluctuation was calculated for each timepoint, timepoints were binned by
cofluctuation, and similarity with time-averaged FC calculated for each bin.
223
224 ***Temporal Spacing Analysis***
225 Our third goal was to compare the effects of different sampling methods on the network
226 structure present in the sampled points. We specifically wanted to investigate the effect of
227 temporal spacing on network structure.
228
Comparison of Sampling Methods
For each subject and session, we examined the network structure present in four groups of time
points: high cofluctuation points (selected as the top 5% of points with highest RSS
cofluctuation), low cofluctuation points (selected as the bottom 5% of points with the lowest RSS
cofluctuation), consecutive points (5% of points selected consecutively beginning at a random
point of the session and wrapping around when needed), and random points (5% of points
selected randomly from the session). For consecutive samples, 100 iterations were done for
each session to not bias the result by starting location. We further tested this by varying the
number of time points selected rather than choosing 5% of time points. The number of time
points was varied from 1 to 100.
239
Circular Offset Analysis
In a supplemental analysis, we examined the relationship between cofluctuation and network
structure after removing temporal spacing effects. To do this, we binned time points by
cofluctuation and then circularly shifted them by 1-10 points in both directions to maintain the
temporal spacing found in the original binning while varying their cofluctuation values. However,
because we previously scrubbed high motion points from this data set, it was not possible to
select 5% of time points (as in other binned analyses) and shift them without running into
scrubbed points. To address this issue, we randomly sampled only 5 points per bin and used
fewer bins (95-100, 85-90, 70-75, 45-50, 20-25, 0-5). This resulted in a smaller number of

analyzed sessions with lower peak similarities for this analysis. To reduce bias from random
sampling, we did 100 iterations and averaged the results.
251
Dataset and Code Availability
MSC data has been made publicly available
(https://openneuro.org/datasets/ds000224/versions/1.0.3). The parcellated timeseries used for
these analyses is available here (https://github.com/GrattonLab/MSC_ROI_data).The code for
the analyses in this paper is available at
(https://github.com/GrattonLab/Ladwig_2022_Events_Static_FC) which will made public upon
publication.
259
260 **RESULTS**
261
Overview:
Previous work showed that moments with high amplitude cofluctuations in BOLD, or "events",
estimate static functional connectivity patterns better than low cofluctuation moments, and can
do so with relatively few timepoints (Esfahlani et al., 2020). This suggested that (1) high
cofluctuation events may be unique, transient phenomena which drive the large-scale network
organization that we observe over long timeseries (Esfahlani et al., 2020). But there are
alternate interpretations of this result: (2) differences between low and high cofluctuation could
be driven by low cofluctuation timepoints exhibiting more BOLD artifacts (e.g., motion or
respiration) that disrupt functional connectivity measures or (3) events may arise as a
consequence of sampling from a continuous distribution, where some moments will, by chance,
exhibit higher cofluctuation than others.
273
274 In this work, we test these three hypotheses. We test how network structure changes over a
275 range of cofluctuation amplitudes, ask if this relationship is present in stationary simulated data,
276 and analyze why events can recreate static correlation structure with so few time points.
277
1. Network structure is continuously related to cofluctuation
First, we examined the relationship between BOLD cofluctuation and network structure across a
range of cofluctuation amplitudes. Our hypotheses are visualized in **Fig. 1A.** If events are
specialized discrete timepoints that drive network structure, then they should especially well
represent network structure (purple) relative to other points. If low cofluctuation points are
discrete timepoints more contaminated by artifacts, they should especially poorly represent
network structure (yellow). If BOLD cofluctuations exhibit random variation as would be
expected from sampling variation, then there should be a continuous relationship between
cofluctuation amplitude and network structure (green).
287
For each participant and resting state session (30 minutes), we calculated BOLD cofluctuation
amplitude at each timepoint (after standard preprocessing and denoising to improve alignment
and remove artifacts, including those associated with motion, see *Methods*). In Esfahlani et al.,
2020, events were defined as the top 5% of timepoints ranked by cofluctuation. We extended
this, grouping timepoints in each session into discrete 5% bins based on their cofluctuation (**Fig.
1B**). For each bin, we calculated an FC matrix using Pearson's correlation **(Fig. 1C)** and
computed measures of network structure as in Esfahlani et al. 2020. **(Fig. 1D-E).**
295
296 We reproduced both results from Esfahlani et al., 2020 showing that compared to FC from the
297 lowest cofluctuation bin ("non-events"), FC from events is more similar to whole-session FC
298 (r_{events} = 0.792, r_{lowest} = 0.514, $t(89)$ = 42.2, p = 1.2e-60) and more modular (q_{events} = 0.562, q_{lowest}
299 = 0.478, $t(89)$ = 12.3 p = 6.0e-21) **(Fig. 1D, E).** However, when we examined the relationship

across intermediate bins, we found that both metrics increased gradually with cofluctuation, not discretely for events. The increase was especially gradual at high values of cofluctuation. In fact, the top bin (events) was not substantially different than the 70th percentile bin (r_{events} = 0.792 vs. r_{70} = 0.797, r_{diff}=-0.005, $t(89)$ = 0.48, p = 0.31; modularity: q_{events} = 0.562 vs. q_{70} = 0.561, qdiff=-0.001, $t(89)$ = 0.15, p = 0.45) and only slightly different than the 50th percentile bin (r_{50} = 0.740, q_{50} = 0.546, r_{diff}=0.052, q_{diff} = 0.016). Low cofluctuation points, while substantially different from events, were not obviously discrete when compared with the 10th and 20th percentile bins (r_{lowest} = 0.514, q_{lowest} = 0.478, r_{10} = 0.579, q_{10} = 0.499, r_{20} = 0.637, q_{20} = 0.515). Notably, many sets of points explicitly excluding events still recapitulate network structure well. These relationships were consistent in all 9 subjects (lines in **Fig. 1D-E**, separated by session in **Fig. S1**), suggesting that neither high nor low cofluctuation points are discrete, specialized, timepoints that drive network structure (or the lack thereof). Rather, network structure appears to be present in all bins, with variability that is positively correlated with the cofluctuation amplitude of a given time point. These results do not suggest that there are a small number of time points which drive functional connectivity.

Fig 1: Network structure varies continuously with BOLD cofluctuation. (A) Previous literature showed that high cofluctuation events contain stronger network structure than low cofluctuation points (gray dots). We posited three hypotheses: (1) high cofluctuation points are discrete phenomena which drive network structure (purple), (2) low cofluctuation points are discrete

artifacts which do not contain network structure (yellow), or (3) there is a continuous gradual
relationship between cofluctuation magnitude and network structure as would be expected from
sampling variability (green). (B) To test these hypotheses, we binned time points into 5
percentile bins of increasing cofluctuation. See example histogram here from MSC05 session 4.
(C) For each bin, we calculated an FC matrix (examples here from MSC02 session 5) and
calculated two measures of network structure – similarity to static FC and modularity. (D)
Similarity to static FC increased gradually with cofluctuation for all subjects (black line = mean,
colored lines = subjects, error bars represent SEM for the group). (E) Modularity increased
gradually with cofluctuation as well. These results suggest that neither high nor low cofluctuation
time points are discrete, unique entities.
330
2. Stationary simulations produce similar behavior to BOLD events and non-events
Above, we found that there was a consistent and gradual relationship between BOLD
cofluctuation amplitude and network structure. Next, we asked, what drives this relationship?
One possible explanation is sampling variability: with noisy data, some timepoints will have
higher similarity to the session average, while others will have lower similarity, simply by
chance. Here, we tested whether sampling variability could account for event behavior by
creating and analyzing a simulated BOLD dataset with stationary covariance structure. In this
simulated dataset, as in the real data in the previous section, we identified points of high and
low cofluctuation and compared their relationship to network structure.
The procedure to generate simulated data is shown in **Fig. 2A**. For each subject and
session, data was generated by sampling from a Gaussian distribution in the dimensionality of
real data. This data was then projected on to the eigenvectors of the static correlation structure
from the real BOLD data for that subject and session, resulting in random Gaussian data with
stationary correlation structure matching real data (see *Methods*).
The analysis from **Figure 1** was repeated on the simulated data. We calculated
cofluctuation for each time point, binned time points by cofluctuation, computed FC matrices for
each bin, and compared the network structure properties across bins.
We found that the relationship between network structure and cofluctuation in simulated
data was remarkably similar to the one found in real data. Similarity to static FC (**Fig. 2B**) and
modularity (**Fig. 2C**) both showed gradually increasing relationships with cofluctuation in the
simulated data, just as in real data. Visually, the network structure present in each bin was
remarkably similar between simulated and real data (**Fig. 2D**). These results were consistent
within individuals and sessions (**Fig S2**). These results suggest that the difference between high
and low cofluctuation moments and their relationship to network structure can be explained by
sampling variability alone. Further, we note that even very simple toy models made from
correlated sine waves and noise show points of high and low cofluctuation amplitude and a
gradually increasing relationship between cofluctuation amplitude and network structure (**Fig.
S3**), indicating this property is not specific to BOLD data.

359
Fig 2: Sampling variability alone can produce event-like behavior. (A) For each subject and
session, we generated a dimensionality-matched timeseries sampled from a Gaussian
distribution. This time series was projected onto the eigenvectors of static FC calculated from
that session. This yielded a simulated random Gaussian data set with BOLD-matched
dimensionality and covariance structure. (B, C) Using the same analysis methods as in Fig 1,
we found that the relationship between network structure and cofluctuation in simulated data
was remarkably similar to the one found in real data. Both (B) similarity with session FC and (C)
modularity increased gradually just as they did in real data. (D) Visually, the FC matrices made
from specific cofluctuation bins look similar between simulated and real data. The data shown is
an example from a single session: MSC02 Session 5. These results suggest the relationship
between network structure and cofluctuation amplitude can be explained by sampling variability
and static FC.
372
3. **Randomly selected timepoints can also reproduce network structure**
One particularly notable property of events is their ability to recapitulate network structure with a
small number of timepoints. As shown in **Fig. 1** and Esfahlani et al., 2020, 5% of time points in a
30-minute resting state session (approximately 1.5 min. of total data) show high similarity with
the static FC calculated from the whole session (r = 0.792). In contrast, past work (Gordon et

al., 2017; Laumann et al., 2015; Noble et al., 2017) suggests that large amounts (> 30 min.) of
resting state fMRI data collection are required to achieve high reliability. This discrepancy
appears to bolster the suggestion that events are discrete transient phenomena which drive
static functional connectivity.
382
383 However, in the previous sections, we showed that events are not unique in their ability to
384 reproduce static FC (**Fig. 1D**). Many other points can recreate static FC. The 70th percentile
385 points were correlated with static FC at r = 0.797 and the 50th percentile points are correlated at
386 r = 0.740. These results raise the question: is the ability for a few points to recreate session FC
387 driven by cofluctuation or something else?
388
We hypothesized that this apparent discrepancy was related to how the events methodology
samples time points. One reason that substantial data is required for reliable FC measures is
because BOLD data is autocorrelated – each time point shares information with the time points
around it. In contrast, the events methodology is not constrained to select temporally adjacent
points. Looking at a sample timeseries, it is obvious that events are more spread out than
consecutive points **(Fig. 3A).** This is confirmed by looking at the histogram of the distance
between events **(Fig. 3B).**
396
To test the effect of temporal spacing on network structure, we compared 5% of points (a)
sampled consecutively (starting from a random section of the scan), (b) sampled randomly
across the whole scan, (c) sampled from the highest cofluctuation points (events), and (d)
sampled from the lowest cofluctuation moments. **Fig. 3C** shows the result: randomly sampled
points are similarly correlated with the static session FC structure as events (r_{random} = 0.78, r_{events}
= 0.79, $t(89)$ = 1.7, p = 0.045). Random points show substantially higher similarity to static
session FC than either low cofluctuation points (r_{low} = 0.50 $t(89)$ = 43.0 p = 1.3e^{-60}), or
consecutively sampled time points ($r_{consecutive}$=0.58, $t(89)$ = 35.2 p = 2.42e^{-54}). These results are
consistent over a range of bin sizes (**Fig. 3D**), suggesting that random temporal spacing is
sufficient to estimate FC well.
407
However, high cofluctuation points are not perfectly matched in spacing to random points
(several occur in close succession relative to what would be expected in a random distribution,
although they are more distributed than a typical consecutive timepoint FC analysis). To
disambiguate the effects of cofluctuation magnitude and temporal spacing, we circularly shifted
the cofluctuation-binned time points (see *Methods*) to keep temporal spacing constant and vary
cofluctuation. We found that after accounting for temporal spacing, there remained a graded
hierarchy where higher cofluctuation points contained more network structure than lower
cofluctuation time points (**Fig. S4**). The simulation results in the previous section suggest that
this is expected and can be parsimoniously explained by sampling variability. Jointly, these
findings suggest that the ability to recreate network structure with a few time points is a function
of both temporal spacing (as shown here) and sampling variability (as shown in the previous
section).

Fig 3: Effects of temporal spacing on estimating FC. (A) Events (red dots) are more temporally spaced than consecutive points, shown here for MSC02 session 6. (B) Histograms of distance between sampled points using consecutive, random, or cofluctuation-based sampling, aggregated over all subjects and sessions. (C) Randomly sampled points are as similar to static session FC as are events; both match static session FC much better than consecutive or low cofluctuation points. (D) These relationships hold over a range of bin sizes. These results suggest that temporal spacing is an important factor in estimating FC well.

DISCUSSION

In this study, we asked if "events", time points with high BOLD cofluctuation, are discrete, transient events that drive functional connectivity. We found that events are not discrete phenomena driving FC. When they are removed, static FC structure is still present. Further, there is a gradual positive relationship between network structure and cofluctuation amplitude, with relatively similar behavior for the top 50% of timepoints, including events. Next, we asked if this gradual relationship between network structure and cofluctuation could be explained by sampling variability on static FC. We created a simulated data set matched to BOLD in dimensionality and covariance structure. Our model produced the same gradual positive relationship seen in real data, including the existence of extreme points like events, suggesting that event behavior can be explained by sampling variability alone. Finally, we analyzed why events are able to recreate static FC with so few points. We found that small numbers of randomly sampled timepoints are also able reproduce static network structure well, suggesting

443   that both sampling variability and temporal spacing are important factors in estimating FC.
444   Taken together, these results support the idea that while events are an especially good
445   representation of the network structure present in static FC, there is not evidence that they are
446   unique points driving it.
447
Should events be used to study the neural underpinnings of functional connectivity?
Although there is a large literature linking fMRI BOLD signal to neural activity (Heeger et al.,
2000; Logothetis et al., 2001), the physiological mechanism of FC itself is incompletely
understood. Past work suggests that BOLD FC is constrained by structural connections (Honey
et al., 2009; Johnston et al., 2008; Vincent et al., 2007) and is related to correlations in neural
activity (Nir et al., 2008; Shmuel & Leopold, 2008; Vincent et al., 2007) but the underlying
drivers of these spontaneous activity correlations remain relatively unknown. Because events
contain similar functional connectivity patterns to static functional connectivity, it was suggested
that these specific moments are responsible for functional connectivity measured over the
timeseries (Esfahlani et al., 2020). From a research perspective, this would make them an
excellent temporal target for investigating the neural mechanism of FC.
459
In this work, we show that while events do match static FC well, they are not discrete markers
for it. When they are discarded, static FC structure is still strongly present in the remaining time
points. Further, there is a gradual and increasing relationship between cofluctuation amplitude
and FC where many points (at least 50%) have a strong relationship with static FC. These
results suggest that events by themselves do not (mechanistically)[1] drive FC and it is unlikely
there is a unique physiological event happening at high cofluctuation points which is creating the
FC matrix. Given these observations, we consider it unlikely that investigating the unique
temporal physiological activity coincident with events would glean additional new information
about the physiologic origins of FC, beyond what might be seen at other timepoints as well.
However, as events show a very strong relationship to FC structure, it is possible that their
study may prove useful for denoising and analysis, to provide a higher signal to noise ratio for
investigations of simultaneous BOLD and direct neural recordings.
472
Relationship between events and static vs. dynamic functional connectivity
Interpretation of events largely depends on one's perspective about the temporal nature of FC.
As has been summarized elsewhere (Lurie et al., 2020), there are two dominant perspectives
on this topic. One perspective posits that functional connectivity exhibits meaningful temporal
dynamics on a moment to moment basis which could represent differences in neural
interactions related to ongoing cognition and task processing (Calhoun et al., 2014; R. M.
Hutchison et al., 2013; Lurie et al., 2020). This view is supported by the fact that there are
transient BOLD responses to tasks (Bandettini et al., 1992; Kwong et al., 1992; Ogawa et al.,
1992), that states can be found in resting-state FC data at second and minute time scales using
sliding windows or instantaneous coactivation patterns (Allen et al., 2014; Chang & Glover,
2010; Petridou et al., 2013; Shakil et al., 2016), and that changes in state properties have been
linked to task behavior, ongoing cognition, and arousal (Chang et al., 2016; Gonzalez-Castillo et
al., 2015; M. R. Hutchison et al., 2013; Kucyi & Davis, 2014; Kupis et al., 2021; Sadaghiani et
al., 2015; Tagliazucchi & Laufs, 2014) as well as more stable measures of cognitive/behavioral
traits and psychiatric disease (Damaraju et al., 2014; de Lacy et al., 2017; Liégeois et al., 2019;
Rashid et al., 2016). From this perspective, static FC is less significant than its constituent parts.
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[1] Events do not appear to drive FC in a unique way but do contribute the most to FC estimates as a mathematical
necessity of their definition and relationship with correlation.

The second perspective posits FC is temporally stable and primarily reflects a history of co-
activation between regions (Laumann & Snyder, 2021). This is supported by evidence that
functional connectivity patterns are consistent within people over sessions (Gratton et al., 2018;
Laumann et al., 2015), only slightly altered during tasks (Cole et al., 2014; Gratton et al., 2016,
2018), and present in anesthesia (Mhuircheartaigh et al., 2010) and slow wave sleep (Sämann
et al., 2011). This perspective emphasizes that resting state FC patterns are only a weak
marker of ongoing cognition, and are instead more related to stable neuroanatomical
constraints, homeostatic processes, and learning related adaptations (Laumann & Snyder,
2021). This perspective collides with the previous one in that it suggests that the dynamic states
found during rest[2] may be explained by sampling variability, motion artifacts, and arousal
(Hindriks et al., 2016; Hlinka & Hadrava, 2015b; Laumann et al., 2017; Liégeois et al., 2017)
rather than current cognitive content or information processing. From this second perspective,
the focus of resting state analysis is on finding a clean and reliable static FC measure that may
be informative about brain organization.
504
The information held in events, then, largely depends on which perspective one takes. From a
dynamic FC states perspective, events help identify states and characterize their properties in a
more temporally specific way. Indeed, events have been used to identify states within resting
state fMRI (Sporns et al., 2021), states that differentiate people (Jo et al., 2021) and states
related to variation in hormone concentrations within individuals across days (Greenwell et al.,
2021). However, from a static FC perspective, events may instead reflect moments of randomly
good representation of the static FC structure. From this view, the previous results could be
interpreted as occurring because events are particularly good timepoints for identifying stable
differences between people and stable static network structure that is relevant to hormonal
neurobiology.
515
Consistent with our findings, Novelli and Razi recently showed that many of the results of edge
functional connectivity (eFC), including the presence of high amplitude cofluctuations, can be
derived from static FC alone (Novelli & Razi, 2021). We showed in this current work that
presence of events and the gradual relationship between cofluctuation and static FC is
predictable from static FC too. While a more extended discussion of dynamic FC is outside the
scope of this work, the results shown suggest that static FC and sampling variability are
sufficient to explain the properties of high cofluctuation timepoints during rest reported so far.
This work alone does not eliminate the possibility of multiple diverse states within resting state
FC. Other modeling work has shown that events arise from biophysical models built on
structural connectivity and simulated spontaneous BOLD signal dynamics (Pope et al., 2021).
However, the present work provides a parsimonious explanation for how events could arise
from a stationary but noisy signal. We echo Novelli and Razi in our interest in future explorations
of edge FC features which cannot be explained by static FC (Novelli & Razi, 2021).
529
Practical considerations for fMRI functional connectivity analysis
Beyond fundamental neurophysiological concerns related to FC, events could be useful for a
range of practical applications in FC analysis. First, we wondered if events could be used to
define a filter for data points particularly suited to FC analysis. And second, given that events
are good at recapitulating static FC, we wondered if it would be possible to reduce data
collection by inducing more event-like time points.
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[2] Significant differences in dynamic FC states are seen with tasks, but they tend to be relatively small (Cole et al., 2014; Gratton et al., 2018; Laumann et al., 2017).

Traditionally, resting state FC analyses try to isolate relevant signal by identifying and extracting
known artifacts (motion, respiration, etc.) and presuming the residual data is all equally useful
(Power et al., 2020). Esfahlani and colleagues' result was particularly exciting because it
suggested that, after addressing artifacts, the remaining data varied in utility for defining FC
structure, with events providing a means to isolate the particularly useful components (Esfahlani
et al., 2020). Although in this paper we showed that events can be explained as a consequence
of sampling variability on static FC, this does not rule out that they may be a useful analytical
tool. In fact, recent work has shown that ETS (edge-time-series) are better at identifying
individuals than static FC (Jo et al., 2021). The strategy of seeking out points with maximal
network information as a 'denoising' strategy is a paradigm shift in fMRI FC analysis and could
be an exciting avenue of future study.
548
The second question is whether the fact that events can recapitulate FC with few timepoints
suggests that FC may be effectively measured through much shorter data collection regimes. It
has become evident in recent years that it is possible to study functional brain organization at
the individual level if enough data is collected (Braga & Buckner, 2017; Gordon et al., 2017;
Laumann et al., 2015; Noble et al., 2017), with most papers suggesting more than 30 minutes of
high quality resting-state data is needed to measure static cortical FC reliably. This has
motivated significant ongoing efforts to collect large amounts of individual 'precision' data
(Fedorenko, 2021; Gratton & Braga, 2021; Naselaris et al., 2021; Pritschet et al., 2021) which
have led to novel findings, but are costly and time-intensive, and may be difficult to acquire in
clinical or pediatric populations. We wondered if, because events contain more network
structure information than other time points, one could decrease data collection by increasing
the rate of events and focusing analysis solely on those moments. However, the results in this
manuscript suggest that event correspondence to static FC can be explained by sampling
variability and spaced sampling – suggesting it would be difficult to ensure a high proportion of
events in a short amount of data collection time. We are optimistic about new strategies for
decreasing data collection needs such as new MRI techniques (Lynch et al., 2020) and efforts
to reduce artifacts (Power et al., 2020) to address these continued issues in fMRI data
collection.
567
Limitations
We will close by noting some limitations in this work and opportunities for future research. First.
we used a dataset collected from a small number of individuals. However, we showed that the
results were very similar across each participant and sessions within participants (Fig. S1),
suggesting robustness in these results. Second, when simulating BOLD data, we used a very
simple model which accounted only for spatial correlation and included no BOLD-like temporal
features (e.g., autocorrelation, matched spectral structure) (Cordes et al., 2001; He et al., 2010;
Liégeois et al., 2021; Zarahn et al., 1997). However, this simple model still was able to produce
event-like behavior, as was an even simpler toy model from sine-waves (Fig. S4). That even
such simple models showed event-like behavior suggests that events arise based on simple
properties of the BOLD timeseries. Third, we focused on resting-state fMRI data in this
manuscript, rather than data from task sessions. We are curious about the effects of tasks on
BOLD cofluctuation: given that arousal and tasks can create real non-stationarities in BOLD
data, we consider it possible that tasks and imposed states could change the prevalence and
structure of events (Betzel et al., 2020; Cole et al., 2014; Gratton et al., 2016, 2018; Laumann et
al., 2017; Tagliazucchi & Laufs, 2014). Future work will be needed to fully explore this issue.
584
Conclusions
In this work, we investigated high cofluctuation BOLD events and found evidence suggesting
that, rather than events behaving as unique discrete timepoints that drive functional

connectivity, events may arise as an expected byproduct of a static functional network structure.
Event recapitulation of network structure was not unique, but varied continuously across
timepoints in real data, and was present in data from which events had been excluded.
Simulations demonstrated similar responses from stationary signals. Finally, one of the primary
interesting properties of events – that they can recreate static FC with a few points – is not
unique and is driven in part by sampling rate. These results suggest that events are
parsimoniously explained as a consequence of a highly correlated, modular, noisy signal
(BOLD) and therefore might be better suited as methods for identifying good representations of
static network structure than as a tool to investigate the mechanistic sources of functional
connectivity.
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ACKNOWLEDGEMENTS
Funding was provided by NIH grant R01MH118370 (CG), NSF CAREER2048066 (CG), the
Washington University Intellectual and Developmental Disabilities Research Center Engelhardt
Family Foundation Innovation Fund (BAS) and NIH T32NS047987 (DMS). This research was
supported in part through the computational resources and staff contributions provided for the
Quest high performance computing facility at Northwestern University which is jointly supported
by the Office of the Provost, the Office for Research, and Northwestern University Information
Technology.

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608 **DECLARATIONS OF COMPETING INTERESTS**
609 None
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CITATION DIVERSITY STATEMENT
Recent work in several fields of science has identified a bias in citation practices such that
papers from women and other minority scholars are under-cited relative to the number of such
papers in the field (Bertolero et al., 2020; Caplar et al., 2017; Chatterjee & Werner, 2021; Dion
et al., 2018; Dworkin et al., 2020; Fulvio et al., 2021; Maliniak et al., 2013; Mitchell et al., 2013;
Wang et al., 2021). Here we sought to proactively consider choosing references that reflect the
diversity of the field in thought, form of contribution, gender, race, ethnicity, and other factors.
First, we obtained the predicted gender of the first and last author of each reference by using
databases that store the probability of a first name being carried by a woman (Dworkin et al.,
2020; Zhou et al., 2020).By this measure (and excluding self-citations to the first and last
authors of our current paper), our references contain 7.04% woman(first)/woman(last), 11.27%
man/woman, 19.72% woman/man, and 61.97% man/man. This method is limited in that a)
names, pronouns, and social media profiles used to construct the databases may not, in every
case, be indicative of gender identity and b) it cannot account for intersex, non-binary, or
transgender people. Second, we obtained predicted racial/ethnic category of the first and last
author of each reference by databases that store the probability of a first and last name being
carried by an author of color (Ambekar et al., 2009; Sood & Laohaprapanon, 2018). By this
measure (and excluding self-citations), our references contain 8.93% author of color
(first)/author of color(last), 12.55% white author/author of color, 28.74% author of color/white
author, and 49.78% white author/white author. This method is limited in that a) names and
Florida Voter Data to make the predictions may not be indicative of racial/ethnic identity, and b)
it cannot account for Indigenous and mixed-race authors, or those who may face differential
biases due to the ambiguous racialization or ethnicization of their names. We look forward to
future work that could help us to better understand how to support equitable practices in
science.
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REFERENCES

Allen, E. A., Damaraju, E., Plis, S. M., Erhardt, E. B., Eichele, T., & Calhoun, V. D. (2014).
Tracking whole-brain connectivity dynamics in the resting state. *Cerebral Cortex (New*
York, N.Y.: 1991), *24*(3), 663–676. https://doi.org/10.1093/cercor/bhs352
Ambekar, A., Ward, C., Mohammed, J., Male, S., & Skiena, S. (2009). Name-ethnicity
classification from open sources. *Proceedings of the 15th ACM SIGKDD International*
Conference on Knowledge Discovery and Data Mining, 49–58.
https://doi.org/10.1145/1557019.1557032
Bandettini, P. A., Wong, E. C., Hinks, R. S., Tikofsky, R. S., & Hyde, J. S. (1992). Time course
EPI of human brain function during task activation. *Magnetic Resonance in Medicine*,
25(2), 390–397. https://doi.org/10.1002/mrm.1910250220
Bertolero, M., Dworkin, J., David, S., Lloreda, C. L., Srivastava, P., Stiso, J., Zhou, D., Dzirasa,
K., Fair, D., Kaczkurkin, A., Marlin, B. J., Shohamy, D., Uddin, L., Zurn, P., & Bassett, D.
(2020). *Racial and ethnic imbalance in neuroscience reference lists and intersections*
with gende. https://doi.org/10.1101/2020.10.12.336230
Betzel, R. F., Byrge, L., Esfahlani, F. Z., & Kennedy, D. P. (2020). Temporal fluctuations in the
brain's modular architecture during movie-watching. *NeuroImage*, *213*, 116687.
https://doi.org/10.1016/j.neuroimage.2020.116687
Bijsterbosch, J. D., Woolrich, M. W., Glasser, M. F., Robinson, E. C., Beckmann, C. F., Van
Essen, D. C., Harrison, S. J., & Smith, S. M. (2018). The relationship between spatial
configuration and functional connectivity of brain regions. *ELife*, 7, e32992.
https://doi.org/10.7554/eLife.32992
Biswal, B., Yetkin, F. Z., Haughton, V. M., & Hyde, J. S. (1995). Functional connectivity in the
motor cortex of resting human brain using echo-planar MRI. *Magnetic Resonance in*
Medicine, *34*(4), 537–541. https://doi.org/10.1002/mrm.1910340409
Braga, R. M., & Buckner, R. L. (2017). Parallel Interdigitated Distributed Networks within the
Individual Estimated by Intrinsic Functional Connectivity. *Neuron*, *95*(2), 457-471.e5.
https://doi.org/10.1016/j.neuron.2017.06.038
Braga, R. M., DiNicola, L. M., Becker, H. C., & Buckner, R. L. (2020). Situating the left-
lateralized language network in the broader organization of multiple specialized large-
scale distributed networks. *Journal of Neurophysiology*, *124*(5), 1415–1448.
https://doi.org/10.1152/jn.00753.2019
Calhoun, V. D., Miller, R., Pearlson, G., & Adalı, T. (2014). The chronnectome: Time-varying
connectivity networks as the next frontier in fMRI data discovery. *Neuron*, *84*(2), 262–
274. https://doi.org/10.1016/j.neuron.2014.10.015
Caplar, N., Tacchella, S., & Birrer, S. (2017). Quantitative evaluation of gender bias in
astronomical publications from citation counts. *Nature Astronomy*, *1*(6), 0141.
https://doi.org/10.1038/s41550-017-0141
Chang, C., & Glover, G. H. (2010). Time–frequency dynamics of resting-state brain connectivity
measured with fMRI. *NeuroImage*, *50*(1), 81–98.
https://doi.org/10.1016/j.neuroimage.2009.12.011
Chang, C., Leopold, D. A., Schölvinck, M. L., Mandelkow, H., Picchioni, D., Liu, X., Ye, F. Q.,
Turchi, J. N., & Duyn, J. H. (2016). Tracking brain arousal fluctuations with fMRI.
Proceedings of the National Academy of Sciences, *113*(16), 4518–4523.
https://doi.org/10.1073/pnas.1520613113
Chatterjee, P., & Werner, R. M. (2021). Gender Disparity in Citations in High-Impact Journal
Articles. *JAMA Network Open*, *4*(7), e2114509.
https://doi.org/10.1001/jamanetworkopen.2021.14509
Cole, M. W., Bassett, D. S., Power, J. D., Braver, T. S., & Petersen, S. E. (2014). Intrinsic and
task-evoked network architectures of the human brain. *Neuron*, *83*(1), 238–251.
https://doi.org/10.1016/j.neuron.2014.05.014

Cordes, D., Haughton, V. M., Arfanakis, K., Carew, J. D., Turski, P. A., Moritz, C. H., Quigley,
M. A., & Meyerand, E. (2001). Frequencies contributing to functional connectivity in the
cerebral cortex in "resting-state" data. *AJNR. American Journal of Neuroradiology*, *22*(7),
1326–1333.
Dale, A. M., Fischl, B., & Sereno, M. I. (1999). Cortical Surface-Based Analysis: I. Segmentation
and Surface Reconstruction. *NeuroImage*, *9*(2), 179–194.
https://doi.org/10.1006/nimg.1998.0395
Damaraju, E., Allen, E. A., Belger, A., Ford, J. M., McEwen, S., Mathalon, D. H., Mueller, B. A.,
Pearlson, G. D., Potkin, S. G., Preda, A., Turner, J. A., Vaidya, J. G., van Erp, T. G., &
Calhoun, V. D. (2014). Dynamic functional connectivity analysis reveals transient states
of dysconnectivity in schizophrenia. *NeuroImage: Clinical*, *5*, 298–308.
https://doi.org/10.1016/j.nicl.2014.07.003
de Lacy, N., Doherty, D., King, B. H., Rachakonda, S., & Calhoun, V. D. (2017). Disruption to
control network function correlates with altered dynamic connectivity in the wider autism
spectrum. *NeuroImage. Clinical*, *15*, 513–524. https://doi.org/10.1016/j.nicl.2017.05.024
Dion, M. L., Sumner, J. L., & Mitchell, S. M. L. (2018). Gendered Citation Patterns across
Political Science and Social Science Methodology Fields. *Political Analysis*, *26*(3), 312–
327. https://doi.org/10.1017/pan.2018.12
Dworkin, J. D., Linn, K. A., Teich, E. G., Zurn, P., Shinohara, R. T., & Bassett, D. S. (2020). The
extent and drivers of gender imbalance in neuroscience reference lists. *Nature*
Neuroscience, *23*(8), 918–926. https://doi.org/10.1038/s41593-020-0658-y
Esfahlani, F. Z., Byrge, L., Tanner, J., Sporns, O., Kennedy, D. P., & Betzel, R. F. (2021). *Edge-*
centric analysis of time-varying functional brain networks with applications in autism
spectrum disorder (p. 2021.07.01.450812). https://doi.org/10.1101/2021.07.01.450812
Esfahlani, F. Z., Jo, Y., Faskowitz, J., Byrge, L., Kennedy, D. P., Sporns, O., & Betzel, R. F.
(2020). High-amplitude cofluctuations in cortical activity drive functional connectivity.
Proceedings of the National Academy of Sciences of the United States of America,
117(45), 28393–28401. https://doi.org/10.1073/pnas.2005531117
Fair, D. A., Miranda-Dominguez, O., Snyder, A. Z., Perrone, A., Earl, E. A., Van, A. N., Koller, J.
M., Feczko, E., Tisdall, M. D., van der Kouwe, A., Klein, R. L., Mirro, A. E., Hampton, J.
M., Adeyemo, B., Laumann, T. O., Gratton, C., Greene, D. J., Schlaggar, B. L., Hagler,
D. J., … Dosenbach, N. U. F. (2020). Correction of respiratory artifacts in MRI head
motion estimates. *NeuroImage*, *208*, 116400.
https://doi.org/10.1016/j.neuroimage.2019.116400
Fedorenko, E. (2021). The early origins and the growing popularity of the individual-subject
analytic approach in human neuroscience. *Current Opinion in Behavioral Sciences*, *40*,
105–112. https://doi.org/10.1016/j.cobeha.2021.02.023
Fulvio, J. M., Akinnola, I., & Postle, B. R. (2021). Gender (Im)balance in Citation Practices in
Cognitive Neuroscience. *Journal of Cognitive Neuroscience*, *33*(1), 3–7.
https://doi.org/10.1162/jocn_a_01643
Glasser, M. F., Sotiropoulos, S. N., Wilson, J. A., Coalson, T. S., Fischl, B., Andersson, J. L.,
Xu, J., Jbabdi, S., Webster, M., Polimeni, J. R., Van Essen, D. C., & Jenkinson, M.
(2013). The minimal preprocessing pipelines for the Human Connectome Project.
NeuroImage, *80*, 105–124. https://doi.org/10.1016/j.neuroimage.2013.04.127
Gonzalez-Castillo, J., Hoy, C. W., Handwerker, D. A., Robinson, M. E., Buchanan, L. C., Saad,
Z. S., & Bandettini, P. A. (2015). Tracking ongoing cognition in individuals using brief,
whole-brain functional connectivity patterns. *Proceedings of the National Academy of*
Sciences, *112*(28), 8762–8767. https://doi.org/10.1073/pnas.1501242112
Gordon, E. M., Laumann, T. O., Adeyemo, B., Huckins, J. F., Kelley, W. M., & Petersen, S. E.
(2016). Generation and Evaluation of a Cortical Area Parcellation from Resting-State

Correlations. *Cerebral Cortex (New York, N.Y.: 1991), 26*(1), 288–303. https://doi.org/10.1093/cercor/bhu239

Gordon, E. M., Laumann, T. O., Gilmore, A. W., Newbold, D. J., Greene, D. J., Berg, J. J., Ortega, M., Hoyt-Drazen, C., Gratton, C., Sun, H., Hampton, J. M., Coalson, R. S., Nguyen, A. L., McDermott, K. B., Shimony, J. S., Snyder, A. Z., Schlaggar, B. L., Petersen, S. E., Nelson, S. M., & Dosenbach, N. U. F. (2017). Precision Functional Mapping of Individual Human Brains. *Neuron, 95*(4), 791-807.e7. https://doi.org/10.1016/j.neuron.2017.07.011

Gratton, C., & Braga, R. M. (2021). Editorial overview: Deep imaging of the individual brain: past, practice, and promise. *Current Opinion in Behavioral Sciences, 40*, iii–vi. https://doi.org/10.1016/j.cobeha.2021.06.011

Gratton, C., Laumann, T. O., Gordon, E. M., Adeyemo, B., & Petersen, S. E. (2016). Evidence for Two Independent Factors that Modify Brain Networks to Meet Task Goals. *Cell Reports, 17*(5), 1276–1288. https://doi.org/10.1016/j.celrep.2016.10.002

Gratton, C., Laumann, T. O., Nielsen, A. N., Greene, D. J., Gordon, E. M., Gilmore, A. W., Nelson, S. M., Coalson, R. S., Snyder, A. Z., Schlaggar, B. L., Dosenbach, N. U. F., & Petersen, S. E. (2018). Functional Brain Networks Are Dominated by Stable Group and Individual Factors, Not Cognitive or Daily Variation. *Neuron, 98*(2), 439-452.e5. https://doi.org/10.1016/j.neuron.2018.03.035

Greenwell, S., Faskowitz, J., Pritschet, L., Santander, T., Jacobs, E. G., & Betzel, R. F. (2021a). *High-amplitude network co-fluctuations linked to variation in hormone concentrations over menstrual cycle* (p. 2021.07.29.453892). https://doi.org/10.1101/2021.07.29.453892

Greenwell, S., Faskowitz, J., Pritschet, L., Santander, T., Jacobs, E. G., & Betzel, R. F. (2021b). *High-amplitude network co-fluctuations linked to variation in hormone concentrations over menstrual cycle* (p. 2021.07.29.453892). https://doi.org/10.1101/2021.07.29.453892

He, B. J., Zempel, J. M., Snyder, A. Z., & Raichle, M. E. (2010). The temporal structures and functional significance of scale-free brain activity. *Neuron, 66*(3), 353–369. https://doi.org/10.1016/j.neuron.2010.04.020

Heeger, D. J., Huk, A. C., Geisler, W. S., & Albrecht, D. G. (2000). Spikes versus BOLD: What does neuroimaging tell us about neuronal activity? *Nature Neuroscience, 3*(7), 631–633. https://doi.org/10.1038/76572

Hindriks, R., Adhikari, M. H., Murayama, Y., Ganzetti, M., Mantini, D., Logothetis, N. K., & Deco, G. (2016). Can sliding-window correlations reveal dynamic functional connectivity in resting-state fMRI? *NeuroImage, 127*, 242–256. https://doi.org/10.1016/j.neuroimage.2015.11.055

Hlinka, J., & Hadrava, M. (2015a). On the danger of detecting network states in white noise. *Frontiers in Computational Neuroscience, 9*, 11. https://doi.org/10.3389/fncom.2015.00011

Hlinka, J., & Hadrava, M. (2015b). On the danger of detecting network states in white noise. *Frontiers in Computational Neuroscience, 9*, 11. https://doi.org/10.3389/fncom.2015.00011

Honey, C. J., Sporns, O., Cammoun, L., Gigandet, X., Thiran, J. P., Meuli, R., & Hagmann, P. (2009). Predicting human resting-state functional connectivity from structural connectivity. *Proceedings of the National Academy of Sciences, 106*(6), 2035–2040. https://doi.org/10.1073/pnas.0811168106

Hutchison, M. R., Womelsdorf, T., Gati, J. S., Everling, S., & Menon, R. S. (2013). Resting-state networks show dynamic functional connectivity in awake humans and anesthetized macaques. *Human Brain Mapping, 34*(9), 2154–2177. https://doi.org/10.1002/hbm.22058

Hutchison, R. M., Womelsdorf, T., Allen, E. A., Bandettini, P. A., Calhoun, V. D., Corbetta, M., Della Penna, S., Duyn, J. H., Glover, G. H., Gonzalez-Castillo, J., Handwerker, D. A.,

Keilholz, S., Kiviniemi, V., Leopold, D. A., de Pasquale, F., Sporns, O., Walter, M., & Chang, C. (2013). Dynamic functional connectivity: Promise, issues, and interpretations. *NeuroImage*, *80*, 360–378. https://doi.org/10.1016/j.neuroimage.2013.05.079

Jo, Y., Faskowitz, J., Esfahlani, F. Z., Sporns, O., & Betzel, R. F. (2021). Subject identification using edge-centric functional connectivity. *NeuroImage*, *238*, 118204. https://doi.org/10.1016/j.neuroimage.2021.118204

Johnston, J. M., Vaishnavi, S. N., Smyth, M. D., Zhang, D., He, B. J., Zempel, J. M., Shimony, J. S., Snyder, A. Z., & Raichle, M. E. (2008). Loss of Resting Interhemispheric Functional Connectivity after Complete Section of the Corpus Callosum. *Journal of Neuroscience*, *28*(25), 6453–6458. https://doi.org/10.1523/JNEUROSCI.0573-08.2008

Kong, R., Li, J., Orban, C., Sabuncu, M. R., Liu, H., Schaefer, A., Sun, N., Zuo, X.-N., Holmes, A. J., Eickhoff, S. B., & Yeo, B. T. T. (2019). Spatial Topography of Individual-Specific Cortical Networks Predicts Human Cognition, Personality, and Emotion. *Cerebral Cortex (New York, N.Y.: 1991)*, *29*(6), 2533–2551. https://doi.org/10.1093/cercor/bhy123

Kucyi, A., & Davis, K. D. (2014). Dynamic functional connectivity of the default mode network tracks daydreaming. *NeuroImage*, *100*, 471–480. https://doi.org/10.1016/j.neuroimage.2014.06.044

Kupis, L., Goodman, Z. T., Kornfeld, S., Hoang, S., Romero, C., Dirks, B., Dehoney, J., Chang, C., Spreng, R. N., Nomi, J. S., & Uddin, L. Q. (2021). Brain Dynamics Underlying Cognitive Flexibility Across the Lifespan. *Cerebral Cortex*, *31*(11), 5263–5274. https://doi.org/10.1093/cercor/bhab156

Kwong, K. K., Belliveau, J. W., Chesler, D. A., Goldberg, I. E., Weisskoff, R. M., Poncelet, B. P., Kennedy, D. N., Hoppel, B. E., Cohen, M. S., & Turner, R. (1992). Dynamic magnetic resonance imaging of human brain activity during primary sensory stimulation. *Proceedings of the National Academy of Sciences*, *89*(12), 5675–5679. https://doi.org/10.1073/pnas.89.12.5675

Laumann, T. O., Gordon, E. M., Adeyemo, B., Snyder, A. Z., Joo, S. J., Chen, M.-Y., Gilmore, A. W., McDermott, K. B., Nelson, S. M., Dosenbach, N. U. F., Schlaggar, B. L., Mumford, J. A., Poldrack, R. A., & Petersen, S. E. (2015). Functional System and Areal Organization of a Highly Sampled Individual Human Brain. *Neuron*, *87*(3), 657–670. https://doi.org/10.1016/j.neuron.2015.06.037

Laumann, T. O., & Snyder, A. Z. (2021). Brain activity is not only for thinking. *Current Opinion in Behavioral Sciences*, *40*, 130–136. https://doi.org/10.1016/j.cobeha.2021.04.002

Laumann, T. O., Snyder, A. Z., Mitra, A., Gordon, E. M., Gratton, C., Adeyemo, B., Gilmore, A. W., Nelson, S. M., Berg, J. J., Greene, D. J., McCarthy, J. E., Tagliazucchi, E., Laufs, H., Schlaggar, B. L., Dosenbach, N. U. F., & Petersen, S. E. (2017). On the Stability of BOLD fMRI Correlations. *Cerebral Cortex (New York, N.Y.: 1991)*, *27*(10), 4719–4732. https://doi.org/10.1093/cercor/bhw265

Liégeois, R., Laumann, T. O., Snyder, A. Z., Zhou, J., & Yeo, B. T. T. (2017). Interpreting temporal fluctuations in resting-state functional connectivity MRI. *NeuroImage*, *163*, 437–455. https://doi.org/10.1016/j.neuroimage.2017.09.012

Liégeois, R., Li, J., Kong, R., Orban, C., Van De Ville, D., Ge, T., Sabuncu, M. R., & Yeo, B. T. T. (2019). Resting brain dynamics at different timescales capture distinct aspects of human behavior. *Nature Communications*, *10*(1), 2317. https://doi.org/10.1038/s41467-019-10317-7

Liégeois, R., Yeo, B. T. T., & Van De Ville, D. (2021). Interpreting null models of resting-state functional MRI dynamics: Not throwing the model out with the hypothesis. *NeuroImage*, *243*, 118518. https://doi.org/10.1016/j.neuroimage.2021.118518

Logothetis, N. K., Pauls, J., Augath, M., Trinath, T., & Oeltermann, A. (2001). Neurophysiological investigation of the basis of the fMRI signal. *Nature*, *412*(6843), 150–157. https://doi.org/10.1038/35084005

Lurie, D. J., Kessler, D., Bassett, D. S., Betzel, R. F., Breakspear, M., Kheilholz, S., Kucyi, A.,
Liégeois, R., Lindquist, M. A., McIntosh, A. R., Poldrack, R. A., Shine, J. M., Thompson,
W. H., Bielczyk, N. Z., Douw, L., Kraft, D., Miller, R. L., Muthuraman, M., Pasquini, L., …
Calhoun, V. D. (2020). Questions and controversies in the study of time-varying
functional connectivity in resting fMRI. *Network Neuroscience (Cambridge, Mass.)*, *4*(1),
30–69. https://doi.org/10.1162/netn_a_00116
Lynch, C. J., Power, J. D., Scult, M. A., Dubin, M., Gunning, F. M., & Liston, C. (2020). Rapid
Precision Functional Mapping of Individuals Using Multi-Echo fMRI. *Cell Reports*, *33*(12),
108540. https://doi.org/10.1016/j.celrep.2020.108540
Maliniak, D., Powers, R., & Walter, B. F. (2013). The Gender Citation Gap in International
Relations. *International Organization*, *67*(4), 889–922.
https://doi.org/10.1017/S0020818313000209
Marcus, D. S., Harwell, J., Olsen, T., Hodge, M., Glasser, M. F., Prior, F., Jenkinson, M.,
Laumann, T., Curtiss, S. W., & Van Essen, D. C. (2011). Informatics and data mining
tools and strategies for the human connectome project. *Frontiers in Neuroinformatics*, *5*.
Scopus. https://doi.org/10.3389/fninf.2011.00004
Mhuircheartaigh, R. N., Rosenorn-Lang, D., Wise, R., Jbabdi, S., Rogers, R., & Tracey, I.
(2010). Cortical and subcortical connectivity changes during decreasing levels of
consciousness in humans: A functional magnetic resonance imaging study using
propofol. *The Journal of Neuroscience: The Official Journal of the Society for*
Neuroscience, *30*(27), 9095–9102. https://doi.org/10.1523/JNEUROSCI.5516-09.2010
Mitchell, S. M., Lange, S., & Brus, H. (2013). Gendered Citation Patterns in International
Relations Journals. *International Studies Perspectives*, *14*(4), 485–492.
https://doi.org/10.1111/insp.12026
Naselaris, T., Allen, E., & Kay, K. (2021). Extensive sampling for complete models of individual
brains. *Current Opinion in Behavioral Sciences*, *40*, 45–51.
https://doi.org/10.1016/j.cobeha.2020.12.008
Newman, M., & Girvan, M. (2004). Finding and evaluating community structure in networks.
Physical Review E, *69*(2), 026113. https://doi.org/10.1103/PhysRevE.69.026113
Nir, Y., Mukamel, R., Dinstein, I., Privman, E., Harel, M., Fisch, L., Gelbard-Sagiv, H.,
Kipervasser, S., Andelman, F., Neufeld, M. Y., Kramer, U., Arieli, A., Fried, I., & Malach,
R. (2008). Interhemispheric correlations of slow spontaneous neuronal fluctuations
revealed in human sensory cortex. *Nature Neuroscience*, *11*(9), 1100–1108.
https://doi.org/10.1038/nn.2177
Noble, S., Spann, M. N., Tokoglu, F., Shen, X., Constable, R. T., & Scheinost, D. (2017).
Influences on the Test-Retest Reliability of Functional Connectivity MRI and its
Relationship with Behavioral Utility. *Cerebral Cortex (New York, N.Y.: 1991)*, *27*(11),
5415–5429. https://doi.org/10.1093/cercor/bhx230
Novelli, L., & Razi, A. (2021). A mathematical perspective on edge-centric functional
connectivity. *ArXiv:2106.10631 [Physics, q-Bio]*. http://arxiv.org/abs/2106.10631
Ogawa, S., Tank, D. W., Menon, R., Ellermann, J. M., Kim, S. G., Merkle, H., & Ugurbil, K.
(1992). Intrinsic signal changes accompanying sensory stimulation: Functional brain
mapping with magnetic resonance imaging. *Proceedings of the National Academy of*
Sciences, *89*(13), 5951–5955. https://doi.org/10.1073/pnas.89.13.5951
Petridou, N., Gaudes, C. C., Dryden, I. L., Francis, S. T., & Gowland, P. A. (2013). Periods of
rest in fMRI contain individual spontaneous events which are related to slowly fluctuating
spontaneous activity. *Human Brain Mapping*, *34*(6), 1319–1329.
https://doi.org/10.1002/hbm.21513
Pope, M., Fukushima, M., Betzel, R. F., & Sporns, O. (2021). *Modular origins of high-amplitude*
co-fluctuations in fine-scale functional connectivity dynamics [Preprint]. Neuroscience.
https://doi.org/10.1101/2021.05.16.444357

Power, J. D., Cohen, A. L., Nelson, S. M., Wig, G. S., Barnes, K. A., Church, J. A., Vogel, A. C.,
Laumann, T. O., Miezin, F. M., Schlaggar, B. L., & Petersen, S. E. (2011). Functional
network organization of the human brain. *Neuron*, *72*(4), 665–678.
https://doi.org/10.1016/j.neuron.2011.09.006
Power, J. D., Lynch, C. J., Adeyemo, B., & Petersen, S. E. (2020). A Critical, Event-Related
Appraisal of Denoising in Resting-State fMRI Studies. *Cerebral Cortex (New York, N.Y.:*
1991), *30*(10), 5544–5559. https://doi.org/10.1093/cercor/bhaa139
Power, J. D., Mitra, A., Laumann, T. O., Snyder, A. Z., Schlaggar, B. L., & Petersen, S. E.
(2014). Methods to detect, characterize, and remove motion artifact in resting state fMRI.
NeuroImage, *84*, 320–341. https://doi.org/10.1016/j.neuroimage.2013.08.048
Pritschet, L., Taylor, C. M., Santander, T., & Jacobs, E. G. (2021). Applying dense-sampling
methods to reveal dynamic endocrine modulation of the nervous system. *Current*
Opinion in Behavioral Sciences, *40*, 72–78. https://doi.org/10.1016/j.cobeha.2021.01.012
Rashid, B., Arbabshirani, M. R., Damaraju, E., Cetin, M. S., Miller, R., Pearlson, G. D., &
Calhoun, V. D. (2016). Classification of schizophrenia and bipolar patients using static
and dynamic resting-state fMRI brain connectivity. *NeuroImage*, *134*, 645–657.
https://doi.org/10.1016/j.neuroimage.2016.04.051
Sadaghiani, S., Poline, J.-B., Kleinschmidt, A., & D'Esposito, M. (2015). Ongoing dynamics in
large-scale functional connectivity predict perception. *Proceedings of the National*
Academy of Sciences, *112*(27), 8463–8468. https://doi.org/10.1073/pnas.1420687112
Sämann, P. G., Wehrle, R., Hoehn, D., Spoormaker, V. I., Peters, H., Tully, C., Holsboer, F., &
Czisch, M. (2011). Development of the brain's default mode network from wakefulness
to slow wave sleep. *Cerebral Cortex (New York, N.Y.: 1991)*, *21*(9), 2082–2093.
https://doi.org/10.1093/cercor/bhq295
Seitzman, B. A., Gratton, C., Laumann, T. O., Gordon, E. M., Adeyemo, B., Dworetsky, A.,
Kraus, B. T., Gilmore, A. W., Berg, J. J., Ortega, M., Nguyen, A., Greene, D. J.,
McDermott, K. B., Nelson, S. M., Lessov-Schlaggar, C. N., Schlaggar, B. L., Dosenbach,
N. U. F., & Petersen, S. E. (2019). Trait-like variants in human functional brain networks.
Proceedings of the National Academy of Sciences, *116*(45), 22851–22861.
https://doi.org/10.1073/pnas.1902932116
Shakil, S., Lee, C.-H., & Keilholz, S. D. (2016). Evaluation of sliding window correlation
performance for characterizing dynamic functional connectivity and brain states.
NeuroImage, *133*, 111–128. https://doi.org/10.1016/j.neuroimage.2016.02.074
Shmuel, A., & Leopold, D. A. (2008). Neuronal correlates of spontaneous fluctuations in fMRI
signals in monkey visual cortex: Implications for functional connectivity at rest. *Human*
Brain Mapping, *29*(7), 751–761. https://doi.org/10.1002/hbm.20580
Smith, S. M., Fox, P. T., Miller, K. L., Glahn, D. C., Fox, P. M., Mackay, C. E., Filippini, N.,
Watkins, K. E., Toro, R., Laird, A. R., & Beckmann, C. F. (2009). Correspondence of the
brain's functional architecture during activation and rest. *Proceedings of the National*
Academy of Sciences, *106*(31), 13040–13045. https://doi.org/10.1073/pnas.0905267106
Smith, S. M., Nichols, T. E., Vidaurre, D., Winkler, A. M., Behrens, T. E. J., Glasser, M. F.,
Ugurbil, K., Barch, D. M., Van Essen, D. C., & Miller, K. L. (2015). A positive-negative
mode of population covariation links brain connectivity, demographics and behavior.
Nature Neuroscience, *18*(11), 1565–1567. https://doi.org/10.1038/nn.4125
Sood, G., & Laohaprapanon, S. (2018). Predicting Race and Ethnicity From the Sequence of
Characters in a Name. *ArXiv:1805.02109 [Stat]*. http://arxiv.org/abs/1805.02109
Sporns, O., Faskowitz, J., Teixeira, A. S., Cutts, S. A., & Betzel, R. F. (2021). Dynamic
expression of brain functional systems disclosed by fine-scale analysis of edge time
series. *Network Neuroscience (Cambridge, Mass.)*, *5*(2), 405–433.
https://doi.org/10.1162/netn_a_00182

Tagliazucchi, E., & Laufs, H. (2014). Decoding wakefulness levels from typical fMRI resting-
state data reveals reliable drifts between wakefulness and sleep. *Neuron*, *82*(3), 695–
708. https://doi.org/10.1016/j.neuron.2014.03.020

Tavor, I., Jones, O. P., Mars, R. B., Smith, S. M., Behrens, T. E., & Jbabdi, S. (2016). Task-free
MRI predicts individual differences in brain activity during task performance. *Science*,
352(6282), 216–220. https://doi.org/10.1126/science.aad8127

van den Heuvel, M. P., Stam, C. J., Kahn, R. S., & Hulshoff Pol, H. E. (2009). Efficiency of
functional brain networks and intellectual performance. *The Journal of Neuroscience:*
The Official Journal of the Society for Neuroscience, *29*(23), 7619–7624.
https://doi.org/10.1523/JNEUROSCI.1443-09.2009

Vincent, J.-L., Patel, G. H., Fox, M. D., Snyder, A. Z., Baker, J. T., Van Essen, D. C., Zempel, J.
M., Snyder, L. H., Corbetta, M., & Raichle, M. E. (2007). Intrinsic functional architecture
in the anaesthetized monkey brain. *Nature*, *447*(7140), 83–86.
https://doi.org/10.1038/nature05758

Wang, X., Dworkin, J. D., Zhou, D., Stiso, J., Falk, E. B., Bassett, D. S., Zurn, P., & Lydon-
Staley, D. M. (2021). Gendered citation practices in the field of communication. *Annals*
of the International Communication Association, *45*(2), 134–153.
https://doi.org/10.1080/23808985.2021.1960180

Yeo, B. T., Krienen, F. M., Sepulcre, J., Sabuncu, M. R., Lashkari, D., Hollinshead, M., Roffman,
J. L., Smoller, J. W., Zöllei, L., Polimeni, J. R., Fischl, B., Liu, H., & Buckner, R. L.
(2011). The organization of the human cerebral cortex estimated by intrinsic functional
connectivity. *Journal of Neurophysiology*, *106*(3), 1125–1165.
https://doi.org/10.1152/jn.00338.2011

Zarahn, E., Aguirre, G. K., & D'Esposito, M. (1997). Empirical analyses of BOLD fMRI statistics.
I. Spatially unsmoothed data collected under null-hypothesis conditions. *NeuroImage*,
5(3), 179–197. https://doi.org/10.1006/nimg.1997.0263

Zhou, D., Cornblath, E. J., Stiso, J., Teich, E. G., Dworkin, J. D., Blevins, A. S., & Bassett, D. S.
(2020). *Gender Diversity Statement and Code Notebook v1.0*. Zenodo.
https://doi.org/10.5281/zenodo.3672110

SUPPLEMENTAL INFORMATION

971
972   **Fig S1, related to Fig 1:** Individual subject results for Fig 1 analyses. In all subjects and
973   sessions, the relationships present between cofluctuation and correlation with time-averaged FC
974   (A) and modularity (B) are continuous, positive, and gradual. It suggests that in all cases,
975   neither high or low cofluctuation time points are discrete. Boxplots show the median, 25th and
976   75th percentile values per subject calculated across sessions.

977
978 **Fig S2, related to Fig 2:** Individual subject results for simulation analysis. In all subjects, the
979 relationships present between cofluctuation amplitude and correlation with time-averaged FC
980 (A) and modularity (B) are continuous, positive, and extremely similar to the relationships
981 present in real data. This suggests sampling variability in static FC is sufficient to explain the
982 presence of high and low cofluctuation points in real data.

983
Figure S3, Related to Fig 2: The relationship between network structure and cofluctuation is
present in extremely simple non-BOLD-like models. We created a 2 network, 4 node model from
sine waves and tested the relationship between network structure and cofluctuation. (A)
Network A is made of two nodes, each with the sine(t) wave. Network B is made of two nodes,
each with sine(t+π/2) wave. Random noise was added to all four nodes. (B) Over the time
course, there is moderately high magnitude (r = 0.7) correlation between in-network nodes. (C)
As in real data, there were points of high and low cofluctuation so it was possible to bin time
points the same way as was done in real and BOLD-simulated data. (D) A similar relationship
exists between cofluctuation and network structure where higher cofluctuation bins are better
able to reproduce network structure from the overall time course. Error bars here represent
SEM over 1000 iterations of the model. (E) This relationship is visually obvious in correlation
matrices. In high cofluctuation bins, the two antagonistic networks are strongly present, and in
low bins there is little or no relationship between nodes.

997
Figure S4, Related to Fig 3: After accounting for spacing, there remains a graded hierarchy of
network structure with cofluctuation. We completed a circular shifting analysis (see *Methods*)
where time points are binned by cofluctuation and then circularly offset. Due to scrubbing, it was
not possible to select as many time points per bin (typically all time points, 5% of total time
points) without running into scrubbed points while circularly shifting the values. To address this
issue, we randomly sampled only 5 eligible points per bin and used fewer bins (95-100, 85-90,
70-75, 45-50, 20-25, 0-5). This resulted in a smaller number of sessions (53/90) which
contained full data for all bin and shift combinations. Because we used only five points,
correlation values (maximum = 0.45 in group data) were much lower than when we calculate
similarity with session FC using 5% of available points. We completed 100 iterations of this
analysis and averaged the results to reduce single trial bias of the random selection of 5 eligible
points. Higher cofluctuation bins have stronger correlation with time averaged FC compared to
their offset counterparts and lower cofluctuation bins have weaker correlation. This suggests
that while temporal spacing does in part drive the similarity of events to static network structure,
there is a relationship between cofluctuation and network structure. Fig 2 suggests this is
parsimoniously explained by sampling variability.