Using predictive validity to compare associations between

brain damage and behavior

John F. Magnotti[1,2], Jaclyn S. Patterson[3], Tatiana T. Schnur[1,3]

1. ttschnur@gmail.com, Department of Neurosurgery, Baylor College of Medicine, Houston, TX, USA

2. john.magnotti@pennmedicine.upenn.edu, Department of Neurosurgery, Perelman School of Medicine at the University of Pennsylvania, Philadelphia, PA, USA

3. jspatter6452@gmail.com, Department of Neuroscience, Baylor College of Medicine, Houston, TX, USA

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Declarations

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CRediT authorship contribution statement

John Magnotti: Conceptualization, Methodology, Formal analysis, Visualization, Software, Writing – original draft.

Jaclyn Patterson: Writing – original draft. Software.

Tatiana T. Schnur: Conceptualization, Methodology, Writing – original draft, Supervision, Funding acquisition.

Abstract

Lesion-behavior mapping (LBM) provides a statistical map of the association between voxel-wise brain damage and individual differences in behavior. To understand whether two behaviors are mediated by damage to distinct brain regions, researchers often compare LBM beta weight outputs by either the overlap method (emphasizing differences) or by the correlation method (emphasizing similarity). However, both methods lack a principled way to determine LBM distinctness and are disconnected from a major goal of LBMs, that of predicting behavior from brain damage. Without such criteria, researchers may draw conclusions from numeric differences between LBMs that are irrelevant to predicting behavior from brain damage. Here, we developed and validated a Predictive Validity Comparison method (PVC) that establishes such a criterion by directly comparing two LBMs based on the difference in predictive accuracy: two LBMs are significantly different if they provide unique predictive power for the two behaviors assessed. Applying the PVC to two lesion-behavior stroke data sets (Ding et al., 2020; Pustina et al., 2018) demonstrated the utility of a statistical criterion for determining when individual differences across behaviors result from the same vs. different lesion patterns. Using region-of-interest based simulations derived from proportion damage in Brodmann regions from a large group of participants (n=131), PVC detected when two behaviors were mediated by different regions (high sensitivity) and determined when two behaviors were mediated by the same region (high specificity). By objectively determining whether two behavioral deficits can be explained by a single vs. distinct patterns of brain damage, the PVC provides a critical advance in establishing the brain bases of behavior. We have released a GUI-driven, open-access web app of this method to encourage widespread adoption.

Introduction

Lesion-behavior mapping (LBM) is used to identify causal relationships between damage to brain regions and behavior (Bates et al., 2003; Rorden et al., 2007). A commonly used application is to determine whether deficits in two behaviors are mediated by damage to the same or different brain areas. Although this type of comparison has been performed extensively in the literature (Alyahya et al., 2021; Arbula et al., 2020; Baldo et al., 2012; Barbey, Colom, Paul, et al., 2014; Barbey et al., 2013; Biesbroek et al., 2016; Binder, Pillay, et al., 2016; Chechlacz et al., 2013; Gläscher et al., 2009, 2010; Harvey & Schnur, 2015; Magnusdottir et al., 2013; Meyer et al., 2016; Mirman, Zhang, et al., 2015; Piras & Marangolo, 2009; Pustina et al., 2018; Rogalsky et al., 2015; Schwartz et al., 2009; Snider et al., 2020; Thye et al., 2021; Zhang et al., 2014b) the field currently lacks a clear criterion to determine whether apparent differences in the LBMs are statistically meaningful.

Identifying the brain regions necessary for human behavior is a well-established scientific endeavor beginning with single-case studies of stroke (e.g., Paul Broca's report concerning patient Tan in 1861), subsequently extending to single case series (Dronkers, 1996; Schwartz & Dell, 2010), and finally gaining increased neural and statistical granularity with the advent of big data voxel-based lesion behavior mapping approaches (Bates et al., 2003; Rorden & Karnath, 2004). Typically, lesions are manually delineated on structural neuroimaging sequences slice-by-slice to create three-dimensional binary representations of the extent and location of brain damage after stroke at the level of the voxel (1-2mm cubed). These lesion masks are normalized to a common brain space to facilitate comparisons between individuals. Next, each voxel is then assessed as to whether its damage is predictive of behavior, similar to a large-scale sparse canonical correlation where every participant has a single behavioral score predicted from the

lesion status of thousands of voxels. Voxels are analyzed either independently in univariate approaches (Bates et al., 2003; Rorden et al., 2007) or in consideration of each other in multivariate approaches (Pustina et al., 2018; Zhang et al., 2014b) cf. Ivanova et al., 2021). Although researchers use these lesion-behavior approaches to identify the brain regions necessary for a single behavior, often we wish to understand whether multiple behaviors are subserved by similar or different brain regions. To date, there are no consistently adopted methods to evaluate whether different behaviors require distinct brain regions through comparing lesion-behavior mapping results, and none which provide a robust statistical criterion.

The most common LBM comparison approach is the Overlap Method (Alyahya et al., 2021; Barbey, Colom, & Grafman, 2014; Biesbroek et al., 2016; Chechlacz et al., 2013; Ding et al., 2020; Gläscher et al., 2019; Harvey & Schnur, 2015; Magnusdottir et al., 2013; Meyer et al., 2016; Mirman, Chen, et al., 2015; Piras & Marangolo, 2007, 2009; Pustina et al., 2018; Snider et al., 2020; Thye et al., 2021; Thye & Mirman, 2018). In this approach, researchers often compare LBMs depicting each behaviors' necessary brain regions (commonly using t-values, beta weights, or voxel cluster size), via intersection. Brain regions represented in one LBM but not the other are interpreted as distinctly involved in that particular behavior, whereas regional intersections are interpreted as regions critical to both behaviors. This technique, however, does not consider the possibility that the differences in LBMs are due to nuisance variance (e.g., sampling error, noise in the behavioral measure, etc.). Further, visual presentations of differences (or intersections) are rarely normalized or compared with a baseline, providing no information as to the scale of the differences, leading to the interpretation that any two LBMs that are not wholly identical are meaningfully different. Therefore, the Overlap method's primary utility is as

a qualitative visualization of the identical (the intersection map) and the non-identical (the

subtraction map) areas of two LBMs.

In contrast, quantitative measures are also used to determine the similarity of LBMs.

Some examples include comparing the number of statistically significant voxels for each region

implicated (Schwartz et al., 2009; Thothathiri et al., 2012), correlating the t-values or beta

weights associated with voxels from two LBMs (Piras & Marangolo, 2009; Zhang et al., 2014b),

and determining the percent of overlapping voxels for each LBM (Binder, Conant, et al., 2016;

Gläscher et al., 2009). While these measures may provide researchers with a certain level of

confidence, the lack of a standardized, statistically rigorous threshold adopted across studies

strongly impedes generalization of brain-behavior relationships. Ultimately, though these

methods provide some quantitative measure of the relationship between two LBMs, none have

an established method for determining a cutoff.

Here, we propose a new statistical method for comparing two LBMs. This technique is

based on the notion of predictive validity: two LBMs are different if and only if they provide

unique predictive power for the two behaviors assessed. This approach is similar conceptually to

comparing the behavioral predictive validity of two methods of neural damage estimation, for

example lesion damage (T1/FLAIR) with functional connectivity (rsfMRI; cf. (Salvalaggio et al.,

2020; Siegel et al., 2016). However, here we developed a method to test whether LBMs fitted to

each behavior are associated with better predictive validity (*i.e.,* a lower Akaike Information

Criterion, AIC) than a "null hypothesis" LBM: an LBM trained on the average of the two

behaviors. If the behaviors were mediated by different brain regions, then this average LBM

should predict both behaviors poorly. This new method provides researchers with a principled

statistical criterion to determine whether observed differences are significantly different *prior* to attempts to explain them.

We assessed our method in two ways. First, we applied the PVC method to real data sets of LBMs generated from different behaviors in stroke populations (Ding et al., 2020; Pustina et al., 2018) and compared the results with overlay and correlation comparison methods. Second, to validate our method, we assessed its ability to correctly identify brain-behavior relationships in two simulations for which the ground truth was known: the two behaviors resulted from damage to different brain regions versus the same brain region. We examined how the distribution of lesion damage across participants impacted the validity of the PVC method. To encourage adoption and extension of this method, we have released an open-source implementation of PVC complete with a user-friendly web-based interface (https://sites.google.com/site/ttschnur/researchprojects/predictive-validity-comparison-for-lesion-behavior-mapping).

Method

The goal of the Predictive Validity Comparison (PVC) method is to determine whether individual differences across two behaviors are the result of a single pattern of lesion damage *vs.* distinct patterns of lesion damage. More concretely, can we accurately predict individuals' behavioral scores using a single lesion-behavior map (LBM) or do we need a distinct LBM for each behavior? We first describe the data used to assess our proposed method and then the details of the PVC method. Next, we use two real datasets (one with highly similar behaviors, one with highly dissimilar behaviors) to compare the PVC method with two common LBM comparison methods: the overlap method and the correlation method. Finally, we provide the results of a simulation analysis that assessed the sensitivity (accurately detecting when two

behaviors have distinct neural bases) and specificity (accurately detecting when two behaviors have a shared neural basis) of the PVC method across changes in two critical parameters: 1) within-region lesion load: the average proportion of damaged voxels within a single region, and 2) between-region lesion load correlation: how strongly proportion damage in one region correlates with proportion damage in another region.

Input data

The Moss Rehabilitation Research Institute (MRRI) Dataset. Lesion volumes and behavioral data for 131 patients (131 total lesion masks, but complete behavior was only available for 130 patients) were generously provided by the MRRI Neuro-Cognitive Rehabilitation Research Patient Registry (reported in previous publications, cf. Mirman et al., 2015; Pustina et al., 2016, 2018; Schwartz et al., 2009, 2011, 2012; Zhang et al., 2014). Patients had chronic left hemisphere stroke and clinical aphasia diagnoses (months post-onset: mean 44, range 2-387 months). All strokes were restricted to cortical infarcts in the left-hemisphere middle cerebral artery territory. Lesion maps were normalized to MNI space and pre-processed as described in (Pustina et al., 2018), available through the LESYMAP R package and ANTs registration (http://stnava.github.io/ANTs/; Avants et al., 2008). Behavioral scores included the Western Aphasia Battery Aphasia Quotient (WAB-AQ; Kertesz, 1982) and accuracy on the Philadelphia Naming Test (PNT; Roach et al., 1996) both reported in Pustina et al. (2018).

The Schnur Laboratory Dataset. We used lesion volumes and behavioral data for 52 subjects consecutively recruited independent of aphasia diagnosis and tested within an average of four days after unique left hemisphere stroke onset (range 1-12 days; reported in Ding et al., 2020). Lesion maps were processed similarly to the MRRI dataset, see Ding et al. We included

two behavioral scores of connected speech, words produced per minute and proportion pronouns to nouns produced during narrative story-telling.

Predictive Validity Comparison

The motivating idea for the Predictive Validity Comparison (PVC) method is that before differences between lesion-behavior maps (LBMs) built from distinct behaviors can be fruitfully interpreted, we must first determine whether the individual differences between the behaviors are better explained by a single LBM *vs*. distinct LBMs. We addressed this question by building two sets of predictions for individuals' behavior. The first set is generated under the null hypothesis: individual differences across the two behaviors are the result of a *single* lesion pattern; the second set is generated under the alternative hypothesis: individual differences across the two behaviors are the result of *distinct* lesion patterns. Only if the quality of the predictions under the alternative hypothesis is higher than under the null hypothesis do we conclude that distinct LBMs should be fit to each behavior. If the quality of the predictions under the null hypothesis is no worse than under the alternative, then we conclude that the data are insufficient to justify fitting distinct LBMs; either the behaviors are mediated by the same underlying lesion pattern or more data are needed to distinguish their individual patterns.

Implementation of the PVC method involved two phases: model building and model comparison. We illustrate each phase using behavioral data simulated from lesions to distinct Brodmann regions (see Method sub-section *Simulating behavior from lesion volumes* for details on the data generating process). PVC was formulated to take advantage of the excellent software toolkit LESYMAP, which provides access to several different lesion behavior mapping techniques. We used SCCAN because of its excellent performance on both real and simulated data, its ability to perform well with typical sample sizes, and its robustness to correlated damage

across regions (Pustina et al., 2018). SCCAN also generates interpretable (sparse) LBMs alongside explicit predicted values for behaviors. We note that other multivariate mapping methods that produce behavioral predictions could also be used with the PVC approach to compare brain damage-behavior associations.

Model Building

In the Model Building phase of the Predictive Validity Comparison (PVC) method, the first step (Figure 1A) is to collect segmented lesion volumes for each subject, aligned within a common coordinate system (*e.g.*, MNI space). Next, the two behavioral scores (B_1, B_2; Figure 1B) are *z*-scored (mean centered, scaled by the standard deviation), producing the normalized behaviors Z_1 and Z_2. Normalization is critical to ensure that simple scale differences between the variables do not influence the lesion-behavior map (LBM) fitting process.

Next, PVC generates multivariate LBMs under the null and alternative hypotheses. In principle, any technique that produces behavioral predictions is amenable for analysis with PVC (*e.g.*, support vector regression); here, we focus on the multivariate LBM technique SCCAN (Pustina et al., 2018) because its approach is explicitly designed to find the maximal (linear) correlation between the lesion volumes and behavior. Under the null hypothesis, individual differences in normalized behaviors Z_1 and Z_2 arise from a single pattern of lesion damage. Therefore, Z_1 and Z_2 measure a single underlying factor and (assuming Z_1 and Z_2 are equally predictive of this underlying factor) can be averaged into a single behavioral score Z_0, which is again *z*-scored (Figure 1C). Lesion volumes and Z_0 are then used to generate a multivariate LBM, denoted LBM_0. In contrast to the null hypothesis, under the alternative hypothesis (Figure 1D), individual differences in behaviors Z_1 and Z_2 arise from distinct lesion patterns and thus PVC creates distinct multivariate LBMs: LBM_1 using the lesion volumes paired with Z_1, (Figure

1D, left) and LBM_2, using the lesion volumes paired with Z_2 (Figure 1D, right). Together, the

PVC method generates three LBMs, one based on the null hypothesis, LBM_0, and two based on

the alternative hypothesis LBM_1 and LBM_2.

Figure 1. Model Building phase in the Predictive Validity Comparison (PVC) Method. **A.** Normalized, segmented lesion volumes for all participants (S_1 to S_n; purple denotes lesioned voxels). **B.** Center and scale (z-scored) behavioral scores (B_1, B_2) prior to fitting for S_1 to S_n (B_1 → Z_1, blue; B_2 → Z_2, orange). **C.** Under the Null Hypothesis (H_0), a single LBM is fit using a single behavior score, Z_0 (z-scored average of Z_1 and Z_2, left) and subject's lesion volume (middle), producing a coefficient for each voxel (scaled from 0 to 1 for display purposes, transparent white to opaque red; right). **D.** Under the Alternative Hypothesis (H_A), distinct LBMs are fit using participants' lesion volumes paired with each scaled behavior Z_1 (LBM_1) and Z_2 (LBM_2).

To ensure the predictions from the LBMs are directly comparable, all hyper parameters must be the same for LBM_0, LBM_1, and LBM_2. For the tests reported here, we chose values based on the real data results and recommendations for best performance from Pustina et al. (2018): sparseness = -0.3 (30% of voxels allowed non-zero beta values; voxel-weights are directional); robust = 0 (do not rank transform input); sparse decomposition iterations = 15. Voxel-weight maps are typically thresholded such that values with less than 10% of the maximum fitted weight are not shown. However, all non-zero voxels are still used in the generation of the predicted behavior scores during model comparison (see *Model Comparison*). The PVC method uses a single (user-controllable) level for sparseness rather than attempting the computationally intensive task of jointly optimizing sparseness across the three datasets. We show (Results sub-section *Sensitivity to hyperparameter choice*) that this choice does not impact the results from the PVC method.

Model Comparison

In the Model Comparison phase (Figure 2), we generate predicted behavior scores using the LBMs from the Model Building phase under both the null (LBM_0) and alternative hypotheses (LBM_1 and LBM_2). For each subject, we take their vectorized lesion volume (Figure 2A) and use the fitted LBMs to make predictions for each behavior. The exact calculations for generating predicted values will depend on the method used for generating the LBMs. In this method, for each LBM fit with SCCAN, the across-subject 0/1 lesion matrix (subjects as rows, voxels as columns) is multiplied by the fitted LBM (a column vector of weights). These predictions are then *z*-scored to convert the predictions to a common scale with the behavioral input. Under the null hypothesis, there is only a single fitted LBM (LBM_0; Figure 2B), and therefore the predicted values for a given subject's normalized behaviors (Z_1 and Z_2) are the same (Figure 2C). That is,

Figure 2. Model Comparison in the Predictive Validity Comparison (PVC) method. **A.** Participants' lesion volumes are multiplied by each fitted lesion-behavior map (LBM) to generate predicted values. **B.** Under the null hypothesis (H_0) there is a single LBM, producing a single prediction ($\hat{Z}_0$) for the two actual scaled behaviors (Z_1, Z_2). **C.** Predictions are compared with the actual scaled behaviors using AIC (solid line indicates equality between predicted and actual values). The total AIC (inset solid bar) for H_0 calculated. **D.** Under the alternative hypothesis (H_A), there are distinct LBMs (LBM_1, LBM_2), producing distinct predictions ($\hat{Z}_1, \hat{Z}_2$) for the two actual scaled behaviors. **E.** Predictions are compared with actual behaviors and total AIC for H_A calculated (inset). **G.** AIC difference ($H_0 - H_A$) determines the winning hypothesis: positive values favor H_A; negative values favor H_0. The gray dashed line at +10:1 is the cutoff for claiming decisive support for H_A.

for subject i, $\hat{Z}_{0i}$ is used to predict both Z_{1i} and Z_{2i}. Total predictive accuracy is summarized using the total Akaike Information Criterion (AIC) across all subjects and both behaviors. Under the alternative hypothesis, the distinct LBMs (Figure 2D) produce distinct predictions across Z_1 and Z_2 for each subject (Figure 2E). AIC is used to measure model fit.

To compare AIC between the null and alternative hypotheses (Figure 2F), we adapted the popular BIC difference thresholds (Kass & Raftery, 1995): AIC differences greater than 10 are *decisive* evidence for the alternative hypothesis (behaviors arise from distinct lesion patterns);

differences between 6 and 10 are taken as s*trong* evidence for the alternative hypothesis.

Negative AIC differences suggest evidence for the null hypothesis (behaviors arise from a single

lesion pattern) and the same cutoffs (now negative differences rather than positive) are used. AIC

difference values between –6 and +6 may be considered *inconclusive* rather than favoring the

null hypothesis because the alternative model has already been penalized for its extra free

parameters (see *Calculating AIC*).

Calculating AIC. Calculating AIC requires choosing a likelihood function and a value for

the penalty term, *k*. First, to estimate the likelihood of the data under each model, we assumed

the normalized behavior scores followed a normal distribution centered on the true behavior with

standard deviation $\sigma = 0.23$. We chose this standard deviation value based on the measured

standard deviation when simulating a single behavioral score with binomial variance. Second, to

determine the penalty term (*k* in the AIC formula), we used the number of uniquely predicted

values. Under the null hypothesis, only a single value is predicted for each subject, therefore *k* is

set to N (where N is the sample size); for the alternative hypothesis the penalty term is 2 * N

because each behavior score was predicted twice. We chose *k* to be based on the number of

predicted subjects rather than the number of fitted voxels because the number of fitted voxels is

affected by choice of hyper-parameters. Additionally, choosing *k* based on the number of

subjects allows us to calculate the relative degrees of freedom between the null and alternative

LBMs independently of the method chosen for fitting them.

Controlling for lesion volume effects. Prior to scaling the behaviors and fitting the LBMs,

the PVC app allows the user to normalize the data based on individual differences in lesion

volume. We suggest scaling the lesion matrix by the square root of total lesion volume (i.e., total

direct lesion volume control; Zhang et al. 2014) rather than regressing out lesion volume from

behavior. As noted by (Thye et al., 2021), regressing out lesion volume from behavior is overly aggressive, as the global lesion volume can be correlated with the lesion volume in the area of interest, leading to false negatives (cf. DeMarco & Turkeltaub, 2018; Sperber, 2022). However, the app provides options for regressing out the lesion volume directly from the behavioral variables, applying both methods, or applying neither. Following Pustina et al. (2018) recommendation for multivariate LBM methods, we default to no lesion volume correction.

Method Assessment

We first compared the accuracy of the Predictive Validity Comparison (PVC) method against the two most popular lesion-behavior map (LBM) comparison methods, the Overlap method and the Correlation method, using real data. Next, we conducted extensive simulations to assess the accuracy of the PVC method using simulated behavior with a known ground truth (behaviors generated from a single *vs*. distinct lesion patterns).

Assessing the PVC method with real data. We compared the output of the PVC method with the Overlap method and the Correlation method using both the MRRI and Schnurlab datasets. Each dataset includes a normalized lesion volume per participant and two associated behaviors for each participant. As a first step, we measured the Pearson correlation between the two behavioral scores to indicate the *a priori* plausibility of being able to distinguish between models predicting each behavior—behaviors that are perfectly correlated should be explainable by a single LBM; uncorrelated behaviors should not be explainable by a single LBM. Next, we used SCCAN to fit multivariate LBMs under the null hypothesis (behaviors arise from a single lesion pattern; LBM_0) and alternative hypothesis (behaviors arise from distinct lesion patterns; LBM_1 and LBM_2). For the Overlap method as is commonly done, we visualized slices of maximal distinction between LBM_1 and LBM_2 but also quantified the degree of similarity with

the Dice coefficient, $\frac{2\times|\text{LBM}_1\cap\text{LBM}_2|}{|\text{LBM}_1|+|\text{LBM}_2|}$: twice the count of non-zero voxels in the intersection of

LBM_1 and LBM_2, divided by the sum of the count of non-zero voxels in each LBM (0.0

indicates no overlap; 1.0 indicates perfect overlap). For the correlation method, we visualized the

non-zero voxel weights for LBM_1 and LBM_2 using a scatterplot and quantified their relationship

using the Pearson correlation. For the PVC method, we visualized the predicted vs. actual

behavior under the null and alternative hypotheses and used AIC difference to select the best-

fitting model.

Assessing the PVC method with simulated data. Because lesion damage varies across

regions and subjects, we examined how the distribution of lesion damage across participants

impacted the validity of the PVC method. For example, if a brain region was only damaged in

one or two participants (i.e., low average lesion load across participants), it is impossible to draw

conclusions about the impact of that brain region on behavior (Kimberg et al., 2007). As a

consequence of low lesion load, it may be difficult to distinguish between LBMs derived from

distinct behaviors: if both LBMs are poor predictors of behavior, they will not have differential

predictive validity (the criterion used by PVC for determining difference). Even assuming lesion

loads are suitably high, if two regions are similarly (un)damaged across participants (high inter-

region damage correlation), the impact of damage to a single of these regions on behavior will be

indiscernible. To estimate the impact of these potential confounding factors on the PVC method

(lesion load and inter-region damage correlation), we conducted extensive simulations using

behavioral data simulated from a real lesion distribution (n=131 lesion volumes from the MRRI

dataset).

For each simulation, we selected two (potentially identical) Brodmann regions and

generated a behavioral score for each participant based on the lesion proportion within each

region. Behavioral scores and lesion volumes were input to the PVC method for analysis. We used the Brodmann atlas provided by LESYMAP for determination of which voxels in MNI space mapped to which Brodmann region. All possible pairs of Brodmann regions in the atlas (41 regions) were included in the simulations, resulting in 820 distinct-region simulations (the alternative hypothesis was true) and 41 same-region simulations (the null hypothesis was true). To assess the impact of average lesion load and inter-region damage correlation on the accuracy of PVC, we separated the simulations based on the within-region lesion load: high-power simulations were defined by at least 10% of patients having at least 5% of voxels damaged in both selected regions; low-power simulations were defined as less than 10% of patients had at least 5% voxel damage to a single region). We then binned regions of interest according to inter-region damage correlation. Any simulation run containing at least 1 region with less than 1% of patients having at least 5% voxel damage was discarded ($n = 158$), leaving 325 high-power simulation runs (300 distinct-region, 25 same-region runs) and 378 low-power simulation runs (366 distinct-region runs, 12 same-region runs).

For the example data shown in Figures 1 and 2, we used the simulation results from Brodmann regions 39 and 40 (see also Supplemental Figure 1). These regions were chosen because they had adequate lesion loads (more than 45% of patients had at least 5% lesion load in each region) and a moderate-to high between-region lesion-load correlation ($r = 0.64$) which reflects real-world usage and non-trivial lesion-overlap.

Simulating behavior from lesion volumes. To generate the behaviors, each simulation assumed behavior scores were linearly related to the proportion of damaged voxels in the region assumed to be responsible for that behavior (100% damage corresponds to 0% accuracy). We refer to this damage proportion as the participant's lesion load for that region. Second, we

assumed scores were probabilistic because of binomial-type noise, that is, the variation in behavior was proportional to the uncertainty of an incorrect *vs*. correct response. Individuals with an expected accuracy near 50% showed more variability than individuals with an expected accuracy near 0% or 100%. This assumption was equivalent to assuming that individuals have a "true" behavioral score (say 75% correct), but varied from this number because of finite sampling, just as a few tosses of a fair coin would not be expected to produce an exactly equivalent number of heads and tails.

Generating behavioral scores for each participant therefore required two steps (repeated for each behavior). First, the true behavior score was set to their lesion load (L) in the selected region. Next, we added noise to the behavioral scores of size e, with $e = s*L*(1-L)$, and s a scaling factor, here set to 1.5. The value 1.5 is not critical for the results, rather it was chosen to produce reasonable amounts of within-subject behavioral variability. No variability ($s = 0$) would eliminate within-subject variation and make determination of "same" LBMs trivial (the behaviors would be identical). Excessive variation would mask any observable relationship between lesion load and behavior. For subjects with 0% or 100% damage to a region, e was set to 0.05 to ensure some minimal amount of variation. This procedure produced scores centered on the true score and ranging from $L - e/2$ to $L + e/2$. Behaviors were then truncated to be within 0 and 1 for all participants.

Output of the PVC method

The PVC application provides several outputs. The behavioral data are output before and after normalization (and lesion-volume-correction if requested) along with the predicted behavioral data as CSV files. The SCCAN-fitted LBMs for B_0, B_1, and B_2 are output as compressed NIFTI files (.nii.gz). The average lesion volume (proportion of patients with damage

at each voxel) and the lesion *mask* volume (thresholded average lesion volume) are also output as compressed NIFTI files. Finally, the input parameters and numeric output are included in a human- and machine-readable YAML file: behavioral variable names, subject identifier, mask threshold, AIC values, SCCAN iteration number, and SCCAN sparseness value. SCCAN voxel directionality is encoded by the sign of the sparseness value where negative indicates "directional" weights (Pustina et al., 2018).

Results

We developed a novel method for determining whether two behaviors are better predicted by a single lesion-behavior map (LBM) *vs*. distinct LBMs. Because of its emphasis on the predictive power of LBMs, we termed the method Predictive Validity Comparison (PVC). We first used two real data sets to assess the practical utility of the PVC method against two most common methods for LBM comparison: the Overlap method and the Correlation method. Next, we used simulated data to determine the sensitivity (correctly detecting when behaviors are generated from distinct lesion patterns) and specificity (correctly detecting when behaviors are generated from a single lesion pattern) of the PVC method.

Assessing the PVC method with real data

MRRI data. We first applied the PVC, Overlap, and Correlation methods to the MRRI data (see Figure 3), which comprised responses from two behaviors, the Western Aphasia Battery Aphasia Quotient (WAB-AQ) and accuracy on the Philadelphia Naming Test (PNT) collected from 130 participants with chronic left-hemisphere stroke. First, we compared the behaviors to determine the *a priori* plausibility of using a single vs. distinct LBMs for explaining the individual variation in each behavior. As shown in Figure 3A, the behaviors were extremely highly correlated across subjects ($r = 0.89$, $p = 10^{-16}$). Under the null hypothesis (H_0) that

individual differences across behaviors arise from a single lesion pattern, we fit a single LBM

(LBM_0) to the average behavior (Figure 3B, *left*). Under the alternative hypothesis (H_A) that

individual differences arise from distinct lesion patterns, we fit two LBMs (LBM_1 and LBM_2),

one for each behavior (Figure 3B, *right*).

The PVC method explicitly compares the LBMs generated from null and alternative

hypotheses. Under the null hypothesis (H_0), a single LBM was fit across behaviors and used to

produce a single predicted value for both the *z*-scored WAB AQ and PNT scores for each

participant. Despite this constraint, predicted values were a reasonable match for the actual

values across participants ($R^2 = 0.42$; Figure 3C). Under the alternative hypothesis (H_A), distinct

LBMs were fit to each behavior and distinct values were predicted for each participant's WAB

AQ and PNT scores; overall accuracy under H_A was also reasonable ($R^2 = 0.45$; Figure 3D). We

used AIC to statistically compare the predictive accuracy of H_0 and H_A, finding decisive support

for H_0: individual differences across WAB AQ and PNT are best explained by a *single* LBM

(AIC Difference = -268, in favor of H_A; Figure 3E).

Both the Overlap and Correlation methods implicitly adopt the alternative hypothesis via

their sole focus on comparing LBM_1 with LBM_2. For the Overlap method, we first visualized the

difference map ($LBM_1 - LBM_2$) to inspect the spatial non-overlap between the fitted LBMs.

Although the fitted LBMs showed some similarity (*cf.* Figure 3B, right) there were also areas of

non-overlap (Dice coefficient = 0.77; Figure 3F). For the Correlation method (Figure 3G), the

correlation between the voxel weights for LBM_1 and LBM_2 was moderate, positive, and

statistically significant ($r = 0.64$, $p = 10^{-16}$).

Figure 3. Comparing lesion-behavior maps (LBMs) built from the MRRI data. **A.** Scatter plot showing the strong linear relationship ($r = 0.89$) between the Western Aphasia Battery Aphasia Quotient (AQ) and the Philadelphia Naming Task (% accuracy) for 130 participants. **B.** Fitted voxel weights (max-scaled across maps; transparent white to opaque red) from LBMs fitted under the null hypothesis (LBM_0) and alternative hypothesis (LBM_1 and LBM_2). The axial slice shown ($z = 107$) had the most non-zero voxel weights for both LBM_1 and LBM_2. LH: Left Hemisphere. **C./D.** The PVC method compares the actual behavior to predictions generated under the null hypothesis (H_0) and the alternative hypotheses (H_A). Solid diagonal line indicates perfect prediction. **E.** The AIC difference was decisive for H_0 (cutoff at -10, gray dashed line). **F.** The Overlap Method highlights slices that differ between the LBMs. Voxel color indicates the sign and magnitude of the difference (opaque blue to transparent white to opaque red; max-scaled). The dice coefficient of 0.77 suggests a moderate to high overlap between the maps. **G.** The correlation method suggested a moderate relationship ($r = 0.64$) between the weights in LBM_1 and LBM_2.

Schnur Laboratory data. Next, we compared the three comparison methods using two

unrelated behaviors calculated from narrative story telling (words produced per minute and

proportion pronouns to nouns) collected from 52 subjects during the acute stage of left

hemisphere stroke (Ding et al., 2020). Unlike the MRRI data, the two behaviors in the Schnur

Lab data had little to no linear relationship (Figure 4A; $r = -0.17$, $p = 0.23$). Under the null

hypothesis that individual differences arose from a single lesion pattern, we fit a single LBM

across behaviors (Figure 4B); for the alternative hypothesis, distinct LBMs were fitted to each

behavior (Figure 4B, right). For the PVC method, the predictions under each hypothesis were

noticeably different. Under the null hypothesis (H_0), the accuracy of the predictions was poor

(Figure 4C, $R^2 = 0.12$), whereas for the alternative hypothesis (H_A), the accuracy was better

(Figure 4D; $R^2 = 0.48$). Even after accounting for the flexibility of fitting distinct LBMs, the

PVC method decisively favored the alternative hypothesis (Figure 4E; AIC difference = 1143, in

favor of H_A). In contrast to the clear result from the PVC method, both the Overlap method and

the Correlation method produced more ambiguous results. For the Overlap method (Figure 4F;

cf. Figure 4B), the difference map showed some distinct regions of non-overlap, but there was

still a moderate degree of overlap (Dice coefficient = 0.52). For the Correlation method, despite

that lack of a behavioral correlation, there was still a significant (albeit small), positive

correlation in the voxel weights ($r = 0.11$, $p = 10^{-16}$).

Figure 4. Comparing lesion-behavior maps (LBMs) built from the Schnur Laboratory data. **A.** Scatter plot showing no linear relationship between z-scored words per min (Speech Rate) and z-scored relative percentage of pronouns for 52 participants. **B.** Fitted voxel weights (max-scaled across maps; transparent white to opaque red) from LBMs fitted under the null hypothesis (LBM$_0$) and alternative hypothesis (LBM$_1$ and LBM$_2$). The axial slices shown (z = 84, 113) had the most non-zero voxel weights for LBM$_1$ and LBM$_2$, respectively. LH: Left Hemisphere. **C./D.** The PVC method compares the actual behavior to predictions generated under the null hypothesis (H$_0$) and the alternative hypotheses (H$_A$). Solid diagonal line indicates perfect prediction. **E.** The AIC difference (H$_0$ – H$_A$ = 1143) used by the PVC method was decisive for H$_A$ (cutoff at +10, gray dashed line). **F.** The Subtraction Method highlights slices that differ between the LBMs. Voxel color indicates the sign and magnitude of the difference (opaque blue to transparent white to opaque red; max-scaled). The dice coefficient of 0.52 suggests a moderate overlap between the maps. **G.** The correlation method assesses the relationship between the weights in LBM$_1$ and LBM$_2$, suggesting a weak but significant positive correlation ($r = 0.11$, $p = 10^{-16}$).

Sensitivity to hyperparameter choice. One source of the flexibility in multivariate LBM fitting methods is the presence of tunable hyperparameters. For instance, SCCAN (Pustina et al., 2018) allows users to set (or optimize) a desired level of sparseness for their data and choose whether to allow voxel weights to have directionality (directional weights allow for positive and negative relationships between lesions and behavior across voxels; non-directional weights assume a fixed direction of relationship across all voxels). Because these hyperparameters affect the fitted weights, they will necessarily affect LBM comparison methods derived from these weights. Therefore, we re-analyzed each of the real data sets using a variety of sparseness levels (in SCCAN, higher levels of the sparseness parameter correspond to *more* voxels included in the fitted LBM) while also varying voxel weight directionality (with and without directionality). Figure 5 shows the data for both the MRRI data set and the Schnur Laboratory data set. Changing sparseness and voxel directionality had no qualitative impact on the results of the PVC method—all tested parameter values showed decisive support for the same hypothesis (H_0 for the MRRI data; H_A for the Schnur Laboratory data). In contrast, the dice coefficient (Overlap Method) and voxel-wise correlation (Correlation Method) showed strong variation across changes in sparseness and voxel directionality. For the MRRI dataset (Figure 5A), the dice coefficient consistently showed medium to high overlap, ranging from 0.49 to 0.95, as the sparseness parameter was increased (more voxels in the map led to increased dice coefficients). However, the voxel-wise correlation ranged broadly from low to high (0.17 to 0.86). For the Schnur Laboratory data set (Figure 5B), the dice coefficient spanned nearly its entire range, from 0.02 to 0.93, as sparseness and voxel directionality varied (more voxels in the map led to increased dice coefficients). The voxel-wise correlation ranged somewhat more narrowly, from 0.03 to 0.39. Such strong variation for these two metrics within and between datasets with

Figure 5. Effect of changing SCCAN sparseness parameter and directionality of voxel weights on lesion-behavior map (LMB) comparison results on real data. Across all sparseness levels (more sparse models have fewer voxels in the resulting LBM; number of non-zero voxels in the null hypothesis LBM are plotted on the horizontal axis) and voxel-weight directionality (pink: directional weights allowed; black: non-negative weights only). **A.** For the MRRI dataset, changing the sparsity of the result had quantitative impacts on the AIC difference used by the predictive validity comparison (PVC) method (Left), but no change in the conclusion (all simulations decisively supported the null hypothesis). For both the subtraction method (Center) and the correlation method (Right), the sparseness of the model modulated the quantitative metrics, but there was little impact of voxel-weight directionality on the results. The Dice coefficient ranged from (0.49 to 0.95) and the voxel-wise correlation ranged from (0.17 to 0.86), obviating the use of a simple threshold for decision as with the PVC method. **B.** For the Schnur dataset, the PVC method showed quantitative differences across parameter manipulations, but no decisional change (all simulations favored the alternative hypothesis). The Dice coefficient from the subtraction method and the voxel-wise correlation from the correlation method were strongly dependent on the choice of sparseness and voxel directionality: the Dice coefficient ranged from (0.02 to 0.93); the voxel-wise correlation ranged from (0.03 to 0.39).

strikingly different behavioral correlations obviates the ability to a derive a single sufficient cutoff value to determine significant similarity between LBM_1 and LBM_2 for either of these methods regardless of hyper-parameter choice. In contrast, the consistency of the PVC method provides a measure of assurance for users that the specific choice of hyper parameters will not drive the result of the LBM comparison.

Assessing the PVC method with simulated data

A primary advantage of the PVC method over the Overlap method and the Correlation method is the ability to set an *a priori* decision threshold for deciding if individual differences across behaviors are better explained by a single *vs.* distinct LBMs. Here, we assessed the accuracy of these decisions from the PVC method by using behavioral scores simulated from the MRRI lesion data. In each simulation, the ground truth is known: the scores were derived from the amount of lesion to distinct Brodmann regions (ground truth different) or from a single Brodmann region (ground truth same). We considered two main lesion distribution characteristics: within-region power (the percentage of individuals with damage to the brain region underlying the specific behavior) and between-region damage correlation (the correlation between the damage within each region across participants; for ground truth same simulations this correlation is always 1.0).

Figure 6 shows the results for the ground truth different simulations. For high-power simulations ($n = 300$), overall accuracy was excellent (282 out of 300 simulations correct; 94% accuracy). The model showed perfect accuracy up to a between-region damage correlation of 0.6 (Figure 6A), then a single error at 0.7 (13/14; 93%) and near floor accuracy with extreme correlations of 0.8 and 0.9 (1/18; 6% correct). For the low-power simulations ($n = 366$), overall accuracy was again excellent (353/366; 96% correct). Errors occurred at a correlation of at least

A. High-power simulations

B. Low-power simulations

Figure 6. Ground truth different simulations. Results for high-powered region pairs (**A**; at least 10% of participants have ≥ 5% damage to *both* regions) and low powered region pairs (**B**; between 1% and 10% of participants have ≥ 5% damage to at least one region). The height of the bars indicates the frequency of simulations classified as correct (AIC > 10; blue), inconclusive (– 10 < AIC < 10; black) or incorrect (AIC < –10; yellow). We binned simulations by the across-subject, between-region % damage correlation (in tenths, from -0.2 to 0.9). The variation in the frequency of high-/low-power region pairs and the frequency of damage correlations was driven by the natural lesion distribution of the MRRI data set.

0.6 (6/9; 67% correct) and increased for extreme correlations, although the sample sizes in this region were small (4/13; 31% correct).

The ground truth same simulations provide an opportunity to consider the false positive rate of the PVC method: given two behaviors that are subserved by the same neural basis (but still differ due to within-subject variability), how likely is the method to claim that distinct maps are needed to accurately predict them? Of the 37 regions that met the minimum-damage inclusion criterion, the false positive rate was perfect for high-power regions (25/25 correct; 0% false alarm rate) and nearly perfect for low-power regions (11/12 correct; 8% false alarm rate).

Discussion

The primary goal of building a multivariate lesion-behavior map (LBM) is to learn the lesion pattern most-predictive of individual differences in a behavior. Often researchers collect two (or more) behaviors from a single cohort and try to determine how LBMs fitted to each

behavior are similar or different. A crucial missing step in this process is determining whether multiple LBMs are, in fact, needed to explain individual differences across the behaviors. We developed the novel Predictive Validity Comparison (PVC) method to fill this gap. The model formalizes the task of picking the appropriate number of LBMs to fit by explicitly comparing the predictive power of a single LBM (predictions generated under the null hypothesis) *vs.* distinct LBMs (predictions generated under the alternative hypothesis). Only after the single LBM predictions are found inadequate (rejecting the null hypothesis) are we justified in interpreting the differences in the lesion patterns learned from fitting distinct LBMs to each behavior. To encourage adoption of our novel PVC method for investigating associations between lesion patterns and behavior, we have released an interactive web-based application (along with all source code) at https://sites.google.com/site/ttschnur/researchprojects/predictive-validity-comparison-for-lesion-behavior-mapping.

Methodological advances

The PVC method offers several advances when applying lesion-behavior-mapping to understand whether different brain regions are necessary for different behaviors. Using two real data sets, we showed that the PVC method was able to make clear decisions in favor of the single *vs.* distinct LBM solutions. These clear results contrasted with the equivocal results from the most common LBM comparison techniques—the Overlap method and the Correlation method. Within the PVC method, there is an established method (difference in AIC) for determining whether two behaviors are better explained by a single *vs.* distinct LBMs. For both the dice coefficient and the voxel-wise correlation, a single threshold is evanescent. For instance, one may try to use the statistical significance of the voxel-wise correlation to determine whether two LBMs are distinct ($p < \alpha$, testing for $r > 0$). However, for both of our real datasets and in our

simulated data, the voxel-wise correlation was statistically different from 0 in nearly all cases. Additionally, the magnitude of the correlation would seem to be relevant: $r = 0.9, p < 0.05$ is certainly better evidence for the equivalence of two LBMs than $r = 0.01, p < 0.05$, but the statistical significance criterion ignores this obvious difference. One may try and choose a cutoff for r to indicate same/different, but there is little principled reasoning for a given value.

Second, the PVC method does not require extensive tuning of hyperparameters (e.g., sparseness, voxel directionality) and is relatively insensitive to their value. In contrast, the Overlap Method (dice coefficient) and Correlation Method are strongly dependent on the choice of LBM fitting parameters, obviating the ability to set a single, principled threshold that works across data sets. For instance, changing the sparseness parameter had drastic effects on the dice coefficient and the voxel weight correlation, but was irrelevant to the ultimate decision from PVC (single vs. distinct LBMs). This difference in sensitivity is caused by the fact that the sparseness parameter has a stronger effect on *which* voxels are selected (affecting the dice coefficient) and on the size of the coefficients (small weights are driven to zero, affecting the voxel weight correlation), but the accuracy itself is largely unchanged. For LBMs with moderate spatial overlap, reducing the number of voxels in each LBM (more sparsity) can increase the perceived difference between the maps without affecting the accuracy of each LBM. This "feature" of the sparseness parameter is why the authors of SCCAN refer to this parameter as controlling the *interpretability* of the solution rather than its *accuracy* (Pustina et al., 2018). Changing sparseness can have a similar effect on the voxel-wise correlation between LBMs—a solution with very few voxels included (more sparse) can induce negative correlations between LBMs that are otherwise positively correlated if more voxels are included (less sparse).

Critically, including or excluding the many small non-zero weights can drastically change the correlation between LBMs without affecting their predictive accuracies.

Third, the PVC method provides excellent specificity and sensitivity in the face of lesion distribution characteristics and several options for accounting for lesion volume. Extensive simulations demonstrated consistently sensitive performance (accurately detecting "different" LBMs) of the PVC method with both low-powered (less 10% of patients having at least 5% damage to the key region) and well-powered (at least 10% of patients have at least 5% damage) lesion loads for damage correlations up to 0.6 (0.7 for well-powered regions). Performance on ground-truth "same" comparisons was high for both low- and well-powered regions.

Advancing theories of brain-behavior associations with PVC

The PVC method provides two specific advantages for testing theories of brain-behavior relationships in comparison to other methods. First, PVC provides a principled method for determining whether a single *vs.* distinct LBMs are needed to explain two behaviors by defining a clear, statistical comparison between these two alternatives: whether the data are fit better by a single *vs.* distinct LBMs. In contrast, the popular Overlap and Correlation methods operate by first assuming what they are trying to prove—that each behavior should be fit by distincts map— and then explaining observed differences. An analogous error would be trying to enumerate all the possible sources of difference between two clinical groups, without first establishing that the two groups are, in fact, statistically different. Avoiding this critical step increases the likelihood of Type I error proliferation and encourages *post hoc* reasoning about group differences. More concretely, an overlap map will nearly always show some spatial differences between LBMs fitted to different behaviors that a clever researcher can explain; however, such spatial differences may be orthogonal to the predictive validity of the LBMs. As we demonstrated here,

the PVC method clearly adjudicates between single *vs.* distinct LBM solutions while the Overlap and Correlation methods are incapable of the same.

We note an additional approach adopted by several laboratories including ours to determine if two brain-behavior relationships are the same is to simply regress out one behavior from another and then use the residuals to fit an LBM (Lukic et al., 2021; Martin et al., 2021; Thye et al., 2021). Here to, this approach fails to construct clear alternatives. The lack of clear alternatives leads to interpretation difficulties when no statistically significant LBMs are produced, and researchers resort to using the Overlap method and interpreting an intersection map. In extreme scenarios, regressing out one variable from another can even induce a spurious relationship between the residuals and brain damage.

A second theoretical advance PVC provides is a more useful map of brain-behavior associations judged to be the same. A typical approach to compare LBMs judged as "same" is to take some combination of them (e.g., intersection, union, average) and interpret the resulting map. However, this approach does not yield a map capable of producing behavioral predictions and does not provide a quantitative comparison between the single-map and distinct-maps solutions. PVC provides the clear decision rule along with a map that is both interpretable and usable for predicting behavior. A related, third advance of PVC is that using the combined behaviors to fit a single, sparse multivariate LBM can reduce nuisance variation in the fitted weights caused by behavioral variability.

Limitations & Future Directions

As with common null hypothesis testing, we should be cautious about "accepting" the null hypothesis. This concern is mitigated somewhat by PVC's use of AIC for model comparison, rather than a strict reliance on p-values that are calculated under the assumption that

the null hypothesis is true (thus rendering it circular to accept the null hypothesis). In formulating the model, we were careful to say "distinct lesion patterns" rather than "distinct *neural bases*" as we recognize that behaviors may indeed have distinct (that is, separate) neural bases, but due to data limitations (poor behavioral measurements, low-quality structural images, correlations in lesion load) are inseparable in a particular data set. For instance, perhaps one of the behaviors under study has no clear relationship with the observed brain lesion pattern, rendering the distinct-maps solution no more accurate than the single-map solution, even though there is no shared neural basis for the behaviors. In this case, inspection of the overall predictive accuracy would provide a clue for correct interpretation. Or, individual differences across two behaviors may be based on damage to two different regions, but if these regions (nearly) always have co-occurring damage in stroke, they will not be statistically separable by any lesion-behavior mapping. One promising approach is to solve this problem is to focus on acute stroke cases, which show smaller lesions (Ding et al., 2020) and may provide better opportunities for dissociating behaviors. Of course, new lesion-behavior data may be able to show the inadequacy of the single-LBM solution (or indeed override previous evidence for the distinct-maps solution). Therefore, it is important to test the predictive validity of fitted LBMs with newly collected data to assess their generalizability.

Although the current formulation of PVC is limited to comparing two behaviors, the idea behind PVC extends naturally to the many-behavior case. PVC simply asks the question: can the behaviors collected be adequately predicted by fewer LBMs than the total number of behaviors. For instance, if you are comparing performance across multiple measures of speech production following brain injury, how many distinct LBMs are necessary to explain a large percentage of variance in the data? One future approach will be to use canonical correlations (the technique at

the heart of SCCAN) to estimate the number of necessary LBMs to explain a given amount of variation in a set of behaviors.

Conclusions

When comparing two lesion behavior maps (LBMs), the most common approaches assume the maps are different and then try to explain any apparent differences. This approach falters by not explicitly testing whether a single LBM predicts both behaviors as well as distinct LBMs. Researchers are left without clear criteria for deciding if the LBMs are different and without a way to estimate a single brain-behavior relationship for behaviors that may have the same neural basis. We developed the Predictive Validity Comparison (PVC) method to overcome these problems. We used both real and simulated data to validate its sensitivity (correctly detecting distinct-LBMs solutions) and specificity (correctly detecting single-LBM solutions). PVC uses a principled statistical criterion to determine if the behaviors are better predicted by a single *vs*. distinct LBMs, and then provides the user with interpretable maps for *either* conclusion. With PVC, researchers can make stronger conclusions about the neural separability of behaviors. We have released an open-source, GUI-driven software toolkit built on LESYMAP and ANTsR that implements the approach (available online at https://sites.google.com/site/ttschnur/researchprojects/predictive-validity-comparison-for-lesion-behavior-mapping).

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Supplemental Information

Simulating behavior from different Brodmann regions

A. Select region pair

LH BA39 and BA40

B. Calculate Lesion Load

S_1 S_2 S_n

	BA39	BA40
S_1	37%	10%
S_2	16%	6%
⋮	⋮	⋮
S_n	36%	39%

C. Simulate Behavior

	B_1	B_2
S_1	52	86
S_2	89	86
⋮	⋮	⋮
S_n	52	28

Simulating behavior from the same Brodmann region

D. Select single region

LH BA39

E. Calculate Lesion Load

S_1 S_2 S_n

	BA39
S_1	37%
S_2	16%
⋮	⋮
S_n	36%

F. Simulate Behavior

	B_1	B_2
S_1	61	58
S_2	93	80
⋮	⋮	⋮
S_n	49	79

Figure S1. Method for simulating lesion-related behavior using Brodmann regions. **A.** To simulate behaviors B_1 and B_2 arising from different Brodmann regions, two region pairs are randomly selected. **B.** Lesion load (L) is calculated for each subject as the proportion of damaged voxels within each region (shown as percentages for display purposes). **C.** Simulated behavior is centered on lesion load, with noise (to mimic within-subject behavioral variability) added proportional to $L \times (1 - L)$, leading to less noise for more extreme lesion loads (near 0 or 1.0). **D.** To simulate behaviors arising from a single Brodmann region, only a single region is selected. **E.** Lesion load is calculated for the single selected region. **F.** Behavior is simulated as in **C**; the only difference between B_1 and B_2 is caused by the added noise component.