Geometrical factors determining dendritic domain intersection between

neurons: a modeling study

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ABSTRACT

Overlap between dendritic trees of neighboring neurons is a defining feature of central nervous systems. Dendritic domains sharing a given locus are arguably more likely to share afferent inputs, and proximity is a requirement for dendro-dendritic communication. Dendritic overlap also differentiates neuronal circuits characterized by redundancy and integration from those characterized by a more specific and selective connectivity. We examined the geometrical factors that affect intersection between pairs of neurons by, specifically, modelling the influence of cell-to-cell distance, and dendritic domain size and shape. We developed MATLAB scripts to determine intersected volume between pairs of three-dimensionally reconstructed neurons using their convex hull (CH) polyhedrons as proxies for dendritic domain. The influence of neuron-to-neuron distance on intersection was not straightforward and reflected the diverse and anisotropic geometry of neurons, and the ostensible displacement of cell bodies from the CH centroid. The influence of size on pair intersection was tested by giving each neuronal CH pair the same (average) volume without modifying their shape. Conversely, the influence of neuronal shape on pair intersection was proved by giving each neuronal pair an average shape without modifying volumes. While both normalization increased intersection, shape averaging was remarkably more effective than size averaging in increasing pair intersection. We conclude that intersection does not only depend on neuron-to-neuron proximity, but critically on neuron-to-neuron differences in size and shape. The results predict that circuits characterized by selective connectivity exhibit greater heterogeneity in size, but especially shape, of their constituent neuronal elements.

Author summary

Neurons communicate with each other using specialized domains called axons and dendrites. Throughout the brain, dendrites from adjacent neurons overlap. This dendritic overlap helps neurons to share common input information coming from axons and also permits communication between dendrites themselves. One way to study dendritic overlap is using the geometrical representation of the dendrites 'field of view', using simplified three-dimensional geometrical shapes (polyhedrons) called convex hulls. In this computational study, we used these convex hulls to analyze the geometrical factors underlying intersection between neurons. For that, we developed methods to obtain the intersected volume of pairs of convex hulls from neurons, to then independently modify the location, size and shape of convex hulls. We observed high variability in intersected volume, even when the neurons were at a similar distance between each other. Relevantly, we also found that variability in volume, but especially variability in convex hull shape is the main factor that determines the degree of intersection between pairs of neurons. These data suggest that differences in dendritic size, but especially differences in shape between neurons have a strong effect on overlap between neurons, and therefore on the potential for neurons to share input information and communicate with each other.

INTRODUCTION

Overlap between the dendritic trees of adjacent neurons is a characteristic found in virtually every region of the central nervous system across vertebrates [1–3]. Neurons whose respective dendrites share a given locus are likely to share common afferent inputs (Peters and Feldman, 1976, as discussed on [5]) and proximity between dendrites is an indispensable condition for synaptic [6,7] or paracrine-volume [8] dendro-dendritic communication. It follows that understanding the factors that influence intersection between adjacent are important to understand how information relay is organized from synaptic afferents to postsynaptic neurons within the brain and also how neurons within a given brain region communicate with each other. Indeed, intersection between adjacent dendritic or axonal fields has been mostly studied in primary neurons of the invertebrate somatosensory system, as well as in various retinal cell types. These studies have provided critical insights on receptive fields development, receptive field functional organization, and cell to cell communication [9–13].

A distinctive feature of the receptive domain of these sensory neurons is its two-dimensional organization, or at least its most relevant functional features. In this work, we wondered about the geometrical factors that affect volume intersection in central nervous system neurons, which in contrast to the above mentioned sensory neurons, have their receptive fields arranged three-dimensionally. Most central exhibit variable and complex geometries and sizes, and the disposition of the dendritic domain in relation to cell body position vary considerably even among neurons of the same type [14–16]. These traits imply that the geometrical determinants of intersection are more complex, and their analysis cannot rely on assumptions of shape circularity

or sphericity. Considering these factors, we sought to answer these simple questions: 1) How

does the shape or size of dendritic domains affect intersection? 2) How does neuron to neuron

proximity affect intersection? 3) How does the location of cell bodies within the dendritic domain

affect intersection?

To address these questions, we used the 3D convex hulls of previously reconstructed neurons

from the ventral tegmental area and substantia nigra [14]. Convex hulls are created joining the

distal points of the dendritic tree to generate a polyhedron that encloses the minimal volume in

which the dendritic domain of the neuron locates and therefore are used as a proxy of dendritic

domain size and shape [14,16–21].

Hence, for this work we set the following aims: 1) to confirm the proof of principle that convex

hull polyhedrons (CHP) are adequate proxies for dendritic space distribution by comparing CHP

volume spatial distribution to dendritic length spatial distribution, 2) to adapt MATLAB scripts

algorithms to estimate the intersecting volume between three dimensional CH, 3) to model the

influence of cell body to cell body mediolateral (ML), dorsoventral (DV) and anteroposterior (AP)

distances on intersected volume, 4) to model the influence of CH size and shape on intersection

by comparing CH pair intersection using original with normalized CH volumes and shapes and,

finally 5) to test whether these methodologies allow us to compare dendritic domain intersection

dynamics between related but segregated populations such as those of the VTA and SNc.

RESULTS

CHP volume and intersection between CHPs pairs problem: method and validation

In this work, we developed methods to determine the intersected volume between the dendritic domain of pairs of adjacent neurons and further studied how the distance between neuronal pairs, as well as the size and shape of each respective dendritic domain affects how much their domains intersect.

A depiction of volume intersection between the dendritic domain of two neurons is shown in Fig 1A. The two reconstructed neurons were placed on their approximate position within the brain tegmentum [14]. When considering the CHP derived from the disposition of dendrites in space (Fig 1B) an intersected volume is defined (Fig 1C, more details in methods).

500 µm

Fig 1. **Dendritic domain intersection.** A) A pair of reconstructed ventral tegmental area dopaminergic neurons (A1) and their corresponding CHPs (A2). Gray volume represents the intersected volume (A3). Cell bodies are represented with discs.

We started by validating the use of CHP as a proxy of the distribution of dendrites in space (Fig 2). For this, we used a sample of 15 tegmental neurons [14]. Specifically, we checked that the extent of a dendritic tree (measured in length) in the space surrounding the cell body (Fig 2A1) was proportional to the convex hull extension (measured in volume) in that particular space (Fig 2A2). For that we performed a wedge analysis (see Methods), dividing the dendritic field of each neuron into 4 anterior and 4 posterior quadrants, as centered on the cell body, and determined the proportion of dendritic length in each of these quadrants. We compared that to the proportion of CHP volume in each respective quadrant (Fig 2B) and found that there were no significant differences between these parameters (Two-way ANOVA Interaction: Anterior quadrants, $F_{(3,42)}=0.4797$ p=0.6981; Posterior quadrants, $F_{(3,42)}=0.6734$ p=0.5732), thus validating the use of CHP as an adequate proxy for the distribution of dendrites in space.

Fig 2. 3D wedge analysis for dendritic length and CHP volume distribution of ventral tegmental area (VTA) neurons. A) Schematic illustrating the 3D wedge analysis, with the cell body placed in the center of a cylinder (blue circle), which is divided into 4 angular wedges (dorsomedial, DM; dorsolateral, DL; ventrolateral, VL and ventromedial, VM) and 2 planes (posterior and anterior planes). The planes run perpendicular to the direction of the cylinder, creating 8 "quadrants". Then, dendritic length is measured in each quadrant and normalized using the total dendritic length of the neuron (A1). For the CHP wedge analysis, the volume of the CHP in each quadrant is measured and normalized by the total CHP volume (A2). Dendrites or CHP edges inside the anterior or posterior plane were colored orange or cyan, respectively. B) Distribution of dendritic

133   trees and CHPs volume for tegmental dopaminergic neurons (n = 15 neurons). When a repeated

134   measures two-way ANOVA was performed within planes and within dendritic length and CHP

135   volume wedge, no significant differences were found: Interaction: $F_{(3,42)}= 0.4797$, p=0.6981 (B1);

136    $F_{(3,42)}= 0.6734$, p=0.5732 (B2). Bars represent mean $\pm$ SEM.

Influence of position, volume and shape on intersected domain: single pair example

We developed scripts to determine the intersected volume between pairs of neuron's CHPs (S1

Fig, see Methods) and then studied the influence of each neuron position and geometry (size and

shape) on intersection. Because the intersected volume depends strongly on the volume of the

individual neurons involved (for instance, at an equivalent distance, the intersected volume of

two large but minimally intersected neurons could be the same as the intersected volume of two

small but largely intersected neurons), it was necessary to find a ratio (IR) that better represented

intersection. We defined this ratio to be the intersected volume divided by the non-intersected

volume. We normalized by the non-intersected volume (and not by the total added volume of

both individual neurons), so that the IR approached 100 (and not 50), for maximally overlapping

CHP.

We measured the IR for all possible pairs of 15 midbrain tegmental neurons as positioned in their

real observed location of their cell bodies within the brain (Montero et al., 2021, see Methods

section). The IR of all possible pairs (105, without repeating pairs) was calculated, and they were

plotted as a function of Euclidian distances between the pair of cell bodies (Fig 3A,B). As

expected, the further away from the cell bodies, the lower the IR. However, high variability in IR

can be observed at equivalent distances between the pairs' cell bodies. As an illustrative example,

Fig 3A shows two neuronal pairs (highlighted in red in 3B) with their respective cell bodies

separated by a similar distance (around 200 μm). Yet the IR of pair A (24.9%) is ostensibly higher

than CHP pair B (1.5%). High variability was also observed when we plotted intersected volume

(mm^3) instead of IR (S2B Fig). These results indicate that IR between neuronal pairs depends on

the distance between their cell bodies, but also on other geometrical characteristics.

Fig 3. IR variability from a sample of tegmental neurons as located in their approximate location

within the brain ventral tegmental area. A) Representative examples of neurons and their CHPs,

as observed from the frontal, lateral and dorsal view. At a similar distance between cell bodies,

CHP pair A showed a higher IR than CHP pair B, respectively. These examples are highlighted in

figure B (red points and letters). Gray volume represents intersected volume. Cell bodies are

represented with discs. B) IR values between pairs of CHPs, as measured in their corresponding

position. Each point represents the IR value of a pair of CHPs (105 pairs tested).

To understand how the differences in geometry between neuronal pairs influence intersection,

we systematically modeled the influence of neuron-to-neuron distance, and neuron-to-neuron

differences in volume and shape, using the cell body as the center of each neuron. Specifically,

we tested how neuron-to-neuron distance influenced IR values when: 1) the original volume and

shape of each neuron were used, 2) the shape of each neuron was maintained but an average

volume was used instead, 3) the volume of each neuron was maintained but an *average* shape

was used, and 4) the average volume and average shape were used for both neurons. We first

modeled a single pair of neurons to illustrate the procedure, but also to study the effect of

distance, volume and shape on intersection in a simpler situation (Figs 4-8). Then, the analysis

was extended to a larger sample of neurons (Fig 9-11).

Fig 4. Original volume - original shape analysis. A-C) A representative example of IR measurement when the distance between pairs of neurons CHPs was 0 µm or 100 µm across the ML (A, frontal view), DV (B, frontal view), and AP (C, lateral view) axis. Cell bodies are represented with discs.

Fig 5. Average volume - original shape transformation and analysis. A) Same pair of CHP as in

Figure 4. Volume was modified for both CHP to 0.045 mm^3 (average value for the pair of neurons).

B-D) IR was measured when the distance between pairs of CHPs was 0 µm or 100 µm across the

ML (B, frontal view), DV (C, frontal view), and AP (D, lateral view) axis. Cell bodies are represented

with discs.

Fig 6. Original volume - average shape transformation and analysis. A) Same pair of CHPs as in

Figure 4 (top row), were aligned around their cell bodies and the average CHP shape was obtained

(cyan, middle row). Using this average CHP, new CHPs were created using the volumes of the

original CHPs (bottom row). B-D) IR was measured when the distance between pairs of CHPs was

0 µm or 100 µm across the ML (B, frontal view), DV (C, frontal view), and AP (D, lateral view) axis.

Cell bodies are represented with discs.

Fig 7. Average volume - average shape transformation and analysis. A) Same pair of CHPs as in

Figure 4 (top row) were aligned around their cell bodies and the average CHP shape was obtained

(middle row, cyan). Using this average CHP, new CHPs were created using a volume of 0.045 mm^3

(average value for the pair of neurons, bottom row). B-D) IR was measured when the distance

between pairs of CHPs was 0 μm or 100 μm across the ML (B, frontal view), DV (C, frontal view),

and AP (D, lateral view) axis. Cell bodies are represented with discs.

Fig 8. Comparison between CHP modeling conditions for a single pair (same as in Figures 4-7).

Effect of distance between cell bodies on IR of the pair of CHPs used in Figures 4-7. IR was

measured between 0 to 400 μm (1 μm steps) within the ML (A1), DV (A2), and AP (A3) axis.

Fig 9. CHP modeling for tegmental neurons: within regions comparison. A) All CHPs of tegmental

neurons used in this study (n = 15, frontal view only). Cell bodies are represented with discs. B)

Analysis for original volume - original shape (OVOS), average volume - original shape (AVOS),

original volume - average shape (OVAS) and average volume - average shape (AVAS) conditions

were performed for all the possible pairs from a sample of tegmental neurons (210 pairs per

distance, except for AVAS, were n=1), and compared within areas. IR was measured between 0

to 400 µm (10 µm steps) within the ML (B1), DV (B2), and AP (B3) axis in each area. Average

volume = 0.047 mm^3 (CHP volume average for nigral neurons). Statistical analyses were

performed using a Friedman test, followed by a Dunn-Sidak post-test. A horizontal line depicts

the significant differences (p<0.05) between OVOS vs AVOS (top black significance lines), OVOS

vs OVAS (top white significance lines) and AVOS vs OVAS (top gray significance lines). Solid line

represents the median. Upper and lower dashed lines represent the 75th and 25th percentile,

respectively (except for AVAS, were n=1). C) Average CHP shape of tegmental neurons, as

observed from the frontal, lateral and dorsal view. Cell bodies are represented with discs.

Fig 10. **CHP modeling for nigral neurons: within regions comparison.** A) All CHPs of nigral

neurons used in this study (n = 15, frontal view only). Cell bodies are represented with discs. B)

Analysis for original volume - original shape (OVOS), average volume - original shape (AVOS),

original volume - average shape (OVAS) and average volume - average shape (AVAS) conditions

were performed for all the possible pairs from a sample of nigral neurons (210 pairs per distance,

except for AVAS, were n=1), and compared within areas. IR was measured between 0 to 400 μm

(10 μm steps) within the ML (B1), DV (B2), and AP (B3) axis in each area. Average volume = 0.042

mm^3 (CHP volume average for nigral neurons). Statistical analyses were performed using a

Friedman test, followed by a Dunn-Sidak post-test. A horizontal line depicts the significant

differences (p<0.05) between OVOS vs AVOS (top black significance lines), OVOS vs OVAS (top

white significance lines) and AVOS vs OVAS (top gray significance lines). Solid line represents the

median. Upper and lower dashed lines represent the 75th and 25th percentile, respectively (except

for AVAS, were n=1). C) Average CHP shape of nigral neurons, as observed from the frontal, lateral

and dorsal view. Cell bodies are represented with discs.

Fig 11. Population analysis of CHP modeling: between regions comparison. Original volume -

original shape (A), average volume - original shape (B), original volume - average shape (C) and

average volume - average shape (D) analysis were performed for all the possible pairs from a

sample of SNc and VTA dopaminergic neurons (210 pairs per distance, except for average volume,

average shape were n=1), and compared between areas. IR was measured between 0 to 400 μm

(10 μm increases) within the ML (A1, D1), DV (A2, D2), and AP (A3, D3) axis in each area. Average

volume = 0.045 mm^3 (CHP volume average of nigral + tegmental neurons). Statistical analyses

were performed using a Wilcoxon rank sum test. A horizontal line depicts the significant

differences (p<0.05) between SNc and VTA. Solid line represents the median. Upper and lower

dashed lines represent the 75th and 25th percentile, respectively (except for AVAS, were n=1).

We started studying intersection (IR) as a function of distance using the original volumes and

shapes of a pair of neurons (original volume – original shape condition). For that, we placed the

cell bodies of the pair of neurons on the origin of a 3D space (coordinate 0, 0, 0), and then

displaced the cell body of one of them 100 μm laterally (Fig 4A), dorsally (Fig 4B) or anteriorly

(Fig 4C) on the ML, DV and AP axes respectively. As it can be observed, IR depended on the axis

on which the neurons were displaced. For instance, the pair in Fig 4 shows over 16% of

intersection at 0 um distance, but when displaced 100 um laterally, dorsally or anteriorly, IR

values change to 23%, 27% and 8%, respectively. It is noticeably that a 100 um separation of cell

bodies in lateral and dorsal directions actually results in higher IR values than when centered

around their cell bodies, illustrating for this pair of neurons and distance tested, the complex

relation between proximity and intersection between neuronal pairs.

We then explored how differences in volume between pairs of neuronal CHP affects IR. We

reasoned that the effect of volume on IR could be studied by controlling for volume, i.e., by

comparing the IR values when original and average volumes were used. We took the same pair

of CHP as in Fig 4 and changed the volume of each neuronal CHP to the average volume between

the two (approximately 0.045 mm^3, Fig 5A). As in Fig 4, we aligned the cell bodies of the same

pair (coordinate 0, 0, 0) and then displaced the cell body of one of them 100 μm laterally (Fig 5B),

dorsally (Fig 5C) and anteriorly (Fig 5D) on the ML, DV and AP axes respectively. We found that

using an average volume resulted in increased IR values lateral or dorsal displacements (as

compared to the original volume - original shape condition, Fig 4) and a slight decrease in IR when

displaced anteriorly.

To address the effect of differences in CHP shape on IR we reasoned that, similarly, this could be

assessed using an *average* shape for both neuronal CHP. We set to find a CHP that, as explained

in detail in the Methods section and S3 Fig, we defined as the CHP of the polyhedron formed by

the points located at mid-distance between the surfaces of two or more CHP, with their cell

bodies aligned. We used the same neurons from Fig 4 and generated the average CHP for this

particular pair. Then, we restored the original volume for each neuron of the pair (Fig 6A). As in

previous figures, we displaced the neuron 100 um laterally, dorsally or anteriorly (Fig 6B-D).

Critically, we found that, in contrast to the original volume - original shape condition (Fig 4) or to

the average volume – original shape condition (Fig 5), using an average shape (while keeping the

original volume) in this pair, a 100 um displacement resulted in IR values that decreased (Fig 6)

in all axes.

Finally, we tested IR using both average volume and average shape (Fig 7, average volume -

average shape). In this case, given that the pair of CHP would be identical, IR was maximal at 0

µm and decreases at 100 um in each axis. Again, in contrast the original volume – original shape

or average volume – original shape conditions, and similarly to the original volume – average

shape condition, all IR values decreased when displaced 100 um, in all axes (Fig 7).

We decided to examine intersection dynamics more systematically by testing the effect of

distance on IR at 0 – 400 um in 1 um steps. In this way, we were able to compare the effect of

volume and shape in terms of distance-versus-IR curves.

As seen in Fig 8 (black curves), the original volume - original shape condition, confirmed that the

relation between IR and CHP position depended on the axis on which the CHP were displaced.

For instance, for this tested pair of CHPs the IR was not decremental for all distances ranges. On

the one hand IR values show a substantial increment for both lateral (ML axis) and dorsal (DV

axis) displacements (hill-shaped or U inverted shape curve), whereas anterior displacement (AP

axis) resulted in a continuous decrement. When testing IR with the neuronal pair having a

common volume (average volume - original shape condition, cyan curves), we observed an

increase in IR values for each tested distance. On the other hand, the overall dependency of IR

to distance (the shape of the curves) was maintained. In contrast, the use of a common shape

(original volume - average shape condition, dark red curves) showed a much more pronounced

effect on distance versus IR curves. To start with, IR curves in ML and DV axes are no longer hill-

shaped and show much higher values at closer distances and in fact, all curves start with an initial

plateau, reflecting that one CHP is inside the other CHP. In other words, normalizing shape not

only increases intersection but, overall, it changes the way intersection depends on distance.

Finally, the use of a common shape and common volume (average volume – average shape

condition, orange curves), which is equivalent to compare two identical CHPs, showed maximal

at 0 µm and a decremental relation for all distances and axes tested.

In summary, these results illustrate the complex relationship between distance and intersection,

reflecting the anisotropic shape as well as the displaced location of the cell body in relation to

the CHPs centroid. Results also suggest that initial shape differences have a much larger effect

than volume differences volume on IR.

323   Influence of position, volume and shape on intersected domain:

324   population analysis

By using a pair of neurons as a representative example, we just described how position, volume,

and shape modifies intersection. To have a more ample view of intersection dynamics within a

brain population, we extended our analysis to 15 neurons of the same tegmental region (the VTA,

Fig 9A) and analyzed their geometry and the rules underlying intersection.

As it can be seen in Fig 9A, we obtained the CHP of those 15 neurons and found that CHPs were

not only diverse in size (Montero et al., 2021) and shape, but also on the location of the cell body

within CHP (circles). In the same way, as for the single pair of neurons shown in Fig 8, we studied

IR as a function of position for all possible pairs for those 15 neurons (210 pairs in total (15 *

(15-1) = 210) this time repeating pairs, because a neuron in a pair was first tested moving to one

orientation of the axis, and then the other).

We first tested the original volume - original shape volume condition (Fig 9B, black curve) and

observed, as expected, that distance decreases IR, yet exhibiting a slight plateau at relatively

close distances (0 – 100 um). Then we tested the average volume – original shape condition using

the average volume of all tegmental neurons sampled (0.047 mm^3, see Methods) and found that

IR increased as tested in the three axes (cyan curves).

In order to provide the average shape, we applied the transformation described for the single

pair of neurons of Figs 6 and 7, but for all tegmental neurons CHPs. The process resulted in an

average shape that is presented in Fig 9C. As it can be appreciated, the average shape exhibits

the essential geometrical features of this dopaminergic population, particularly the dendritic

domain size and the extension in the ML, DV and AP axes. In frontal view, we observe that the

CHP was oriented dorsomedially to ventrolaterally, with the cell body at mid position, in

agreement with the distribution of VTA neurons dendritic field, as described in (Montero et al.,

2021). We confirmed that distribution of volume around the cell body for this average CHP was

equivalent to that found for all CHPs in the wedge analysis from Fig 2 (Anterior: DM=11.06%,

DL=4.82%, VL=14.54%, VM=6.60%; Posterior: DM=17.76%, DL=7.78%, VL=26.75%, VM=9.80%).

Fig 9B (dark red curves) shows the effect that averaging shape (original volume – average shape)

has on distance versus IR curves, which show much higher values than both the original volume

– original shape and average volume – original shape conditions, in the three axes tested. The

average volume – average shape condition, as also observed in Fig 8 for the single CHP pair,

showed maximal values at every distance and axis tested.

We extended our analysis to a related population of neurons and examined whether intersection

dynamics were similar. For that, we took 15 nigral neurons (Montero et al., 2021) and obtained

their CHP (Fig 10A). We confirmed that CHP was a good proxy for dendritic distribution in nigral

neurons, repeating the wedge analysis of Fig 2 and found that volume distribution for individual

CHP did not differ from dendritic length distribution (S4A Fig, Two-way ANOVA interaction: SNc

Anterior quadrant, $F_{(3,42)}$=0.2566 p=0.8562; SNc Posterior quadrant, $F_{(3,42)}$=0.9138 p=0.4425). We

confirmed high variability in IR values as a function of Euclidian distances from the real observed

location of nigral neurons within the brain (Montero et al., 2021, see Methods section). As for

tegmental neurons (Fig 3A and B), the IR of all possible pairs of nigral neurons (15 * (15 − 1)) / 2)

= 105) was calculated, and they were plotted as a function of Euclidian distances between the

pair of cell bodies (S4B,C Fig), indicating, again, that geometrical factors have a great influence

on intersection. Finally, we also obtained the average CHP (Fig 10C) and found the typical

dorsolateral to ventromedial orientation of nigral neurons [14] and the cell body displaced

medially, while its location seems to be more central regarding AP position (seen in frontal and

lateral views), in agreement with the described distribution of nigral neurons dendritic field (S4A

Fig). Relevantly, average CHP volume wedge for nigral neurons, was similar to the values found

for dendritic length and CHP volume wedge from S4A Fig (Anterior: DM=5.86%, DL=12.92%,

VL=19.16%, VM=10.43%; Posterior: DM=5.47%, DL=20.04%, VL=19.93%, VM=5.20%).

Results showed that IR curves dynamics of IR curves in the 3 axes for nigral neurons were similar

to VTA tegmental neurons (Fig 10B). Interestingly, original volume – original shape (black curves)

exhibited a slight but consistent IR maximal near 100 um, similar to what was observed for the

single pair example of Fig 8. For average volume computations, the average CHP volume for our

sample of nigral neurons was 0.042 mm^3. Similar to VTA neurons, we also observed that

averaging shape (dark red curves) increased IR values when compared to the original volume –

original shape condition, but especially compared to the average volume – original shape

condition (cyan curves). Thus, these results confirm that CHP shape variability is the main factor

determining IR between neuronal pairs.

Intersection dynamics between tegmental and nigral populations

Finally, we compared tegmental and nigral populations in each of the four tested conditions (Fig

11). For original volume - original shape condition (Fig 11A), tegmental neurons showed higher

IR values than nigral neurons at shorter distances in the ML and DV axis and across all the tested

distances in the AP axis, while at larger distances between cell bodies, nigral neurons showed

higher IR values than tegmental neurons in ML and DV axis.

Regarding average volume - original shape, some differences were evidenced between the two

populations (Fig 11B). Here, we obtained the average CHP volume taking together both nigral

and tegmental neurons values, with the value being equal to 0.045 mm^3. Although for VTA

tegmental neurons IR values were higher than nigral neurons in ML and DV, they were observed

at fewer distances than in original volume - original shape condition. Moreover, nigral neurons

showed significant differences at more distances than VTA at larger distances compared to

original volume - original shape condition. Regarding the AP axis, VTA neurons continued to show

higher IR values than nigral neurons in all tested distances.

In the original volume - average shape condition, both populations showed higher IR values than

in the average volume - original shape condition, yet curves for both areas were similar in the ML

and DV axes (Fig 11C). Regarding the AP axis, VTA neurons still showed higher IR values than SNc

in all tested distances.

Finally, in the average volume - average shape condition, considering that only one pair of CHPs

is tested, differences between areas were assessed by testing whether in each axis the data fitted

to the same curve or not (Fig 11D). In this case, an exponential decay model was applied. In each

axis, higher R^2 values (>0.99) were found when the data of each area was fitted alone than when

data of both tegmental and nigral populations were pooled together. This means that, for each

axis, a significant difference between curves was found. Then, our results showed that in ML and

DV axes, the nigral population curves were higher than tegmental neurons curves, whereas the

tegmental neurons curve was higher than the nigral curve in the AP axis.

Overall, these results highlight that differences in CHP shape and position allow to determine

differences in intersection between the dendritic fields of differentiated brain populations

(tegmental VTA and nigral SNc) dopaminergic neurons.

DISCUSSION

In this study we developed computational tools to estimate the volume generated by the intersection of two adjacent neurons' dendritic domains. Using CHPs as a proxy for dendritic domain size and shape, we modeled the effect of neuron-to-neuron proximity in a three-dimensional space and the effect of dendritic domain volume and shape of individual neurons on intersection. Our results show that the rules governing geometrical intersection between neurons are complex, reflecting the anisotropic shape of neuron's dendritic domain as well as the displaced location of the cell body inside it. Results also show that differences in dendritic domain size, but especially differences in its shape increase exclusion (i.e. decrease intersection) between adjacent neurons. In the following sections, we discuss the methodological challenges involved in this study as well as the biological significance of these findings.

Computational tools to find an intersected region have been developed before for pairs of convex polygons [22,23] and polyhedrons [22,24,25]. Yet to the best of our knowledge this is the first attempt to use these tools to study overlap in 3D-structured neurons. In fact, with few exceptions [26,27], studies on overlap between nervous structures have been carried out on peripheral somatosensory or visual systems neurons, focusing on the (2D) surface covering properties of receptive fields formed by dendrites or nerve terminals [11]. In addition, studies have usually focused on the average overlap between neurons of a receptive field [9,10,12,13], but not on the specific geometrical properties that finally determine receptive field overlap for a given population. Thus a first step in this work was to develop tools to determine the intersected

volume between CHPs efficiently (S1 and S5 Figs), which in turn allowed us to model the effects

of 3D geometry on intersection.

In order to study the influence of shape on intersection (see below), an additional challenge in

this study was to find an average shape of two or more CHP which fulfilled the need of being

theoretically sensible and practically useful. We defined the average CHP as the CHP of a

polyhedron formed by the points located at mid-distance between the surfaces of two or more

CHP with their cell bodies aligned. The solution evokes that of graphic morphing or

metamorphosis used in computational graphics to provide smooth transition between two

different shapes using intermediate steps [28–31]. In that sense, the average CHP could be seen

as analogous to an intermediate step shape. The difference between the morphing approach and

ours, however, is that in some morphing approaches specific (correspondent) points are defined

as *a priori* landmarks and can work as a pivot (for instance the eyes when morphing from one

face to another) [32], whereas in our solution the there are no landmarks to pivot on. Thus, our

intermediate step shape can be seen as a true *average shape*.

The use of neurons' convex hull to represent dendritic distribution poses the question of the

extent to which it represents a meaningful proxy for dendritic domain size, shape, or even

function in 3D space. In fact, the vast majority of space within a neuronal CHP is not occupied by

dendritic segments. We tackled this question by comparing dendritic length with that of convex

hull volume, as it distributes around the cell body. We found that dendritic length and CHP

volume distributions were indistinguishable from each other, supporting the conclusion that

CHPs are adequate proxies for dendritic distribution at least for our population of tegmental and

nigral neurons.

Overlap between dendritic fields of neighboring neurons is a widely occurring phenomenon in

the central nervous system of vertebrates [1–3]. Studying the intersection between dendritic

trees of neurons is important for understanding how a neuronal system is organized. For

instance, proximity between dendritic trees is an obvious requirement for synaptic dendro-

dendritic communication, such as that occurring between olfactory neurons [7] or midbrain

dopaminergic neurons themselves [6]. Proximity is also a requirement for dendro-dendritic

communication mediated by the dendritic release of neurotransmitters, which are subjected to

uptake or degradation following release, as in the case of dendritic dopamine [8] or acetylcholine

release from brainstem neurons [33,34], respectively. Evidence also supports the parsimonious

idea that dendrites sharing a given locus share the same synaptic inputs (Peters and Feldman,

1976, as quoted in [5]). From this argument, it follows that systems in which the dendritic domain

of constituent neurons overlap extensively may be characterized by sampling connectivity

(archetypical of reticular or brainstem core neurons) and those in which dendritic domains tend

to avoid overlap, may be conversely characterized by a selective input strategy (more typical of

specific sensory systems) [3,35,36].

As mentioned, intersection has been mostly studied for neurons in which the receptive field

(dendritic or axonal) is two-dimensional, and these studies have focused on determining the

average area of receptive fields overlap (or not) with neighboring neurons at the population level

using the coverage factor or other meaningful ratios [11]. On the other hand, few studies have

examined the geometrical determinants of dendritic fields overlap [37]. We used 3D convex hulls,

which for the most part have been used to characterize and classify neuronal populations by CHP

shape or size [17–21,38–40], to study dendritic domain intersection between central neurons.

Our results show that in addition to cell-to-cell distance predictably decreasing intersection,

distance versus intersection relationship was not straightforward and had to depend on other

geometrical factors. Indeed, intersection was affected by the relative position of each neuron to

its pair (i.e. whether one locates besides, above/below, or in front/behind from the other). This

is an expected consequence of the dendritic domain of neurons not being spherical (i.e. they are

anisotropic) in that maximal extensions in ML, DV or AP axes differ from each other. Indeed, one

could argue that differences in intersection curves between tegmental and nigral populations

(Fig 11) can be explained by differences in each axes extension (Fig 9B, 10B). The location of the

cell body, which we used to identify each neuron "position" and showed ostensible displacement

from the dendritic domain's centroid, was also a relevant factor influencing intersection

dynamics. Indeed, as seen for the representative example (Fig 8), but also for many neurons in

the population (see IR curves for original volume – original shape in Fig 10) intersection ratio was

maximal when cell bodies were located some distance apart, not close, from each other. This is

an interesting result that challenges the intuitive assumption that neurons whose cell bodies are

located next to each other should have a maximal chance of sharing afferents inputs.

Perhaps the most remarkable prediction of this study, however, is the finding that dendritic

domain intersection is significantly increased by size, and especially shape, homogeneity

between neurons (Fig 8, 9 and 10). Or, said conversely, that dendritic domain exclusion between

adjacent neurons is significantly increased by heterogeneity in dendritic domain size and shape.

The broad spectrum of dendritic domain arrangements among neuronal types has been

conceptualized as representing different types of connectivity, either of the selective, sampling

or space filling type. The former type is characterized by small dendritic fields occupying a

restricted locus, and represents an efficient solution to relay nervous signals from one neuronal

stage to another as parallel, separate channels. The sampling strategy (and to some extent the

space filling's) connectivity strategy, on the other hand, is characterized by broader dendritic

fields encompassing different loci, and represents a solution to increase integration and

redundancy in signal transferring [3]. Our results allow us to predict that for systems in which

transfer of nervous signal requiring parallel and exclusive transferring of signals may be also

accomplished by heterogeneity in both size, but specially shape of dendritic domains.

METHODS

Animals, single neuron labeling and reconstruction

Reconstructed dopaminergic neurons came from a pool of previously reported neurons [14,41,42]. Neurons were labeled with Neurobiotin using juxtacellular or intracellular labeling methods and brain tissue was processed to reveal Neurobiotin and tyrosine hydroxylase to confirm the dopaminergic profile. Next, neurons were manually reconstructed using Neurolucida (MBF Bioscience) from confocal image stacks (more details in Montero et al., 2021). The somatodendritic domain was completely filled, shrinkage corrected and reconstruction tilted-corrected. For some analyses, individual neuronal reconstructions were placed in a custom-made 3D map of substantia nigra and VTA based on [43], according to the ML, DV, and AP location of the cell body.

Shape of CHP

To obtain the actual shape of CHP of an individual neuron, the *convhulln* function in MATLAB was used. The *convhulln* function is based on Quickhull algorithm from Barber et al., 1996, which allows the obtain the smallest CHP from a given set of points. The input for the *convhulln* function was the *Segment points-dendrites* data from Neurolucida, which contains the 3D coordinates of each dendritic segment (S1A Fig, column 1). The outputs of *convhulln* are the list of vertices that form a facet and the volume of the CHP (S1A Fig, column 1). The volumes of CHPs obtained using *convhulln* coincided with the volumes reported for CH by Neurolucida Explorer (MBF Bioscience) (Montero et al., 2021).

Intersected volume methods

Obtaining the volume of the intersected polyhedron required a transformation of the way the

CHPs were encoded. For that, we tested 3 methods, which are summarized in S1 Fig. As stated

previously, the segment points from a reconstructed neuron were used to obtain the CHP (S1A

Fig, column 1). For method 1, we added a 3D grid of points using the *ndgrid* function of MATLAB

(1 µm distance between points) to a cuboid formed by the maximal ML, DV, and AP extensions

of the neuron CHP (S1A Fig, column 2) and, using the *inhull* function (D'Errico 2021, S1A Fig,

column 3), obtained the 3D grid of points that located inside the CHP. We confirmed that the

obtained volume corresponded to the original measured volume using the *convhulln* function.

For method 2, we added the same 3D grid of points using the *ndgrid* function of method 1, but

instead of selecting those points inside the hull, we selected only those points from the 3D grid

that were in touch with the CHP facets (S1A Fig, column 3). Again, we confirmed that the obtained

volume corresponded to the *convhulln* function volume. For method 3, we started from the

original CHP and obtained the vertices (S1A Fig, columns 1 and 2). By using the *linspace* function,

vertices forming each CHP facet were joined using 1000 points per CHP edge (S1A Fig, column 3).

Thus, we ended with three transformed CHP defined by either: (1) points filling the CHP volume,

(2) points covering the CHP facets and (3) points lined up along edges. These three different ways

of encoding CHPs were tested for finding the intersected polyhedron volume between a pair of

CHPs

Using method 1 (points filling the CHP), for a given pair of CHP points, the common points

between the pair of CHPS were obtained using the *intersect* function. Intersected points were

then used to obtain a CHP using *convhulln*, and the intersected volume in mm^3 was obtained (S1B

Fig, first row). For method 2 (points covering facets), the points of each CHP facet that are inside

the other CHP were found using the *inhull* function. Again, with these outputs of points, the

intersected CHP can be calculated using *convhulln* and the intersected volume measured (S1B

Fig, second row). With method 3 (points lining up edges), the procedure is similar to method 2:

using the *inhull* function, the points from each CHP edge that are inside the other CHP of the pair

are obtained, and then the *convhulln* function is used to obtain the intersected CHP and the

intersected volume (S1B Fig, third row). While all three methods allowed to obtain a similar

intersected volume, big differences were found regarding the time required to complete the

intersection calculation. Using a sample of 15 SNc dopaminergic neurons and testing all the

possible pairs without repeating reciprocal distances (105 pairs of CHPs in total), method 1

showed a mean calculation time per pair of CHP of 68.18 $\pm$ 3.51 sec, followed by method 2, with

9.06 $\pm$ 0.38 sec. Method 3 was the fastest of the three methods, with a mean calculation time of

0.21 $\pm$ 0.01 sec. Considering that method 3 was the fastest without losing accuracy, this method

was used in all the following analyses.

Wedge Analysis

We used the 3D wedge function from Neurolucida Explorer software. In this analysis, the

distribution of the processes as they extend from the centroid of the cell body in every direction

is obtained. To achieve this, the neuron is placed in the center of a cylinder, which in this study

was divided into 4 angular wedges, and in 2 parallel planes perpendicular to the direction of the

cylinder, with the division of the planes centered in the cell body. For instance, if the cylinder is

placed parallel to the anteroposterior axis, the four angular wedges report the location of the

processes in the dorsomedial, ventromedial, ventrolateral, and dorsolateral quadrants, at each

of the 2 planes defined in the AP axis (Fig 2A1, S4A Fig). Results were presented as a percentage

of the total dendritic length in each quadrant. A similar procedure was used to analyze the wedge

from CHPs (CHP wedge analysis, Fig 2A2, S4A Fig). This analysis was performed using a custom

MATLAB script. In this case, the percentage of the total CHP volume was determined in each

quadrant of the anterior and posterior planes. A further CHP wedge analysis was carried out for

SNc and VTA average CHP shapes (explained above).

Intersecting ratio. It was reasoned that because the intersected volume depends strongly on the

volume of individual CHP neurons (for instance, the intersected volume of two large but

minimally intersected neurons could be the same as the intersected volume of two small but

largely intersected neurons), it was necessary to find a ratio that normalized for the volume. As

such it was decided to work with an intersection ratio (IR), that is defined as follows:

$$Intersection\ Ratio = \frac{Intersected\ Volume}{Non\_intersected\ Volume} \: x \: 100$$

$$Non\text{-}intersected\ Volume = CHP\ Volume\ 1 + CHP\ Volume\ 2 - Intersected\ Volume$$

For example, the pair of CHPs in S5A Fig exhibit a larger intersected volume than the pair of CHPs

in S5B Fig, but when each intersected volume is divided by their corresponding non-intersected

volume, the IR is comparable between these two pairs of CHPs. We decided to normalize by the

non-intersected volume, and not by the total added volume of both individual neurons, so that

the ratio approaches 100 (and not 50), for maximally overlapping CHP. In any event, the results

in the vast majority of analysis did not vary between ratios using either the *non-intersected*

volume or the *total added volume* as divisors (not shown), nor when total intersected volume

was used.

Method for change CHP volume

Using a custom MATLAB script, CHP volume can be modified by multiplying the CHPs vertices

coordinates by the following conversion factor:

619
$$\sqrt[3]{\frac{New\ CHP\ volume}{Original\ CHP\ volume}}$$

The converted CHPs conserve their shape and the position of their cell body. We used this

procedure to change the analyzed sample of neurons to a new CHP volume that corresponded

to the average between the CHP volumes of a pair of neurons (Figs 5 and 7), the average of

tegmental (Fig 9) or nigral (Fig 10) neurons, and the average of tegmental + nigral (Fig 11)

neurons.

Method for determining CHP average shape

To address the effect of CHP shape on IR, we needed first a rationale and then a method to define

an average CHP in 3D. The chosen rationale can be narrated as follows: let's imagine an apex

centered at 0, 0, 0 and from which rays emanate in all directions in space. Then the somatic

centers of a pair of CHP are placed at the apex (as shown in Fig 6, see also S3 Fig). Any single ray

will intersect the facets of the two CHP at distances d1 and d2. Then, a point at mid-distance

between d1 and d2 is defined, and the exercise is repeated for all rays emanating from the apex.

A new polyhedron will be created by all points located at mid-distance between the facets of

both CHP at every solid angle. This procedure can be projected to a larger number of CHP

neurons, in which case the points of the new polyhedron will correspond to the average of all n

distances at which rays intersect the facets of all CHP in a given ray direction.

Explained in detail, the procedure is based on a surface-to-point transformation procedure. It

starts placing the somatic center of a CHP on the center of a Cartesian space (0, 0, 0) where the

three orthogonal axes (ML, DV and AP) intersect. Then, a plane (e.g. AP – ML plane) orthogonal

to one axis (DV) is chosen, and the distances from the center to the CHP facets in that plane are

measured. This is repeated 360 times in 1-degree steps, in an anticlockwise direction. That

defines a polygon formed by 360 points (S3 A1-5 Fig). To move from that polygon to a 3D

polyhedron, the original plane is systematically tilted in 1-degree steps around a new axis (e.g.

the ML axis). That creates a polyhedron with 64800 points on its surface (S3 A6-10 Fig). To obtain

a CHP average from a given number of CHPs, the transformed CHPs were centered in the origin,

using the somatic center as a reference point. Then, the mid-distance between analogous points

on the surface of their respective CHP was determined. A simplified 2D explanation for the

average process of 2 or 15 convex hull polygons is provided in S3A and B Figs, respectively. It

should be noticed that a consequence of this procedure is that the resulting polyhedron (or

resulting polygon in the simplified 2D explanation of S3A and B Figs)) is likely not to be convex all

around its surface (S3A Fig), for which an approximate convex hull must be defined using the

convhulln function. On the other hand, the more CHP are included, the more similar is the

resulting polyhedron to its convex hull (S3B Fig).

Computational and statistical analysis

659 MATLAB R2018a was used on a Lenovo P51 (Intel i7-7820HQ, 16 Gb of RAM, NVIDIA Quadro

660 M1200) with Windows 10. Statistical analyses were performed on MATLAB. Two-way ANOVA

661 was used (Fig 2B, S4A Fig). Friedman test followed by Dunn-Sidak post-test and Wilcoxon rank

662 sum test were performed (Figs 9-11). An exponential decay model was used when required (Fig

663 11D). Significance for all statistical tests was set at $p < 0.05$.

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S1 Fig. Methods to quantify the intersected volume between CHPs. A) CHP transformation

methods. We started using the dendritic segment points from a digitally reconstructed neuron

(blue points, top left diagram). The cell body is represented with a disc. Then, the CHP from the

neuron was obtained (blue lines, middle left diagram). Following, a grid of points was generated

around the CHP (red points), on a grid equal to the maximal extension of the CHP in the ML, DV

and AP axis (middle center diagram). Grid points separation = 1 µm. Next, the points of the grid

that were inside of the CHP were determined (blue points, top center diagram). For method 1,

the points located inside the CHP were used (top right diagram). For method 2, the points from

the grid that were touching the CHP facets were used (middle right diagram). For method 3, the

vertices from the CHP (blue open circles, bottom center diagram), were used to define the CHP

edges linking the CHP vertices using points (1000 points per edge, bottom right diagram). B) CHP

intersection quantification methods. A pair of CHPs was tested to obtain the intersected volume

using the transformed CHP with the three methods described in (A). With method 1, the

intersected points from each grid of CHPs were obtained. Using method 2, the points from the

surface of the first CHP that were inside the second CHP were obtained, and conversely the points

from the surface of the second CHP that were inside the first CHP were obtained. For method 3,

the points from the edges of the first CHP that were inside the second CHP were obtained, and

conversely the points from the edges of the second CHP that were inside the first CHP were

obtained. The calculated intersected volume for each method was similar (Method 1= 0.024

mm^3; Method 2= 0.025 mm^3; Method 3= 0.024 mm^3). However, differences were found in the

time spent to calculate the intersection (for a sample of 105 pairs of SNc CHPs, Method 1 = 68.18

$\pm$ 3.51 sec; Method 2 = 9.06 $\pm$ 0.38 sec; Method 3= 0.21 $\pm$ 0.01 sec).

S2 Fig. Intersected volume from a sample of CHP from SNc and VTA dopaminergic neurons.

Measurement of the intersected volume between pairs of CHPs from SNc (A) and VTA (B), as

measured in their corresponding position in each area. A total of 105 pairs of CHPs were tested

in each area. Each point represents the intersected volume value of a pair of CHPs.

S3 Fig. Simplified 2D representation of average shape computation. A) Average shape method

explained for a pair of 2D CH polygons. The polygons were centered in the origin in relation to

their cell body, and a line is plotted at 0 degrees. The average point from the sample of 2 points

in the given angle was obtained (black open circle, A1). Next, the process was repeated at 1-

degree steps (A2-A5). Finally, 360 points were obtained, that were transformed to the average

CHP shape using the *convhulln* function (A6). B) Average shape method explained for a group of

15 2D polygons. CHPs were centered in the origin (B1) and the average of the points in each angle

were obtained (B2). Then, the average CHP shape was calculated using the *convhulln* function

(B3). Scaling is different for examples B and C.

S4 Fig. IR variability from a sample of nigral neurons. A) Distribution of dendritic trees and CHPs

volume for nigral neurons (n = 15 neurons). When a repeated measures two-way ANOVA was

performed within planes and within dendritc length and CHP volume wedge, no significant

differences were found: Interaction, $F_{(3,42)}$= 0.2566, p=0.8562 (A1); $F_{(3,42)}$= 0.9138, p=0.4425 (A2).

B) Representative examples of nigral neurons and their CHPs, as observed from the frontal,

lateral and dorsal view. At a similar distance between cell bodies, CHP pair A shows a much higher

IR than CHP pairs B. These examples are highlighted in figure B (red points and letters). Gray

volume represents intersected volume. Cell bodies are represented with solid circles. C)

Measurement of the IR between pairs of CHP from SNc, as measured in their corresponding

position in each area. Each point represents the IR value of a pair of CHPs.

S5 Fig. Using IR to normalize the intersected volume between pairs of CHPs. Two examples of

CHP intersection are shown (A1-A2). The pairs of neurons show a different intersected volume,

but a similar IR. Gray volume represents intersected volume.

A1 A2 A3

500 μm

Fig 1

A1 Dendritic length wedge

A2 CHP volume wedge

B1 Anterior quadrants

B2 Posterior quadrants

Fig 2

Pair A
24.9%

Pair B
1.5%

500 μm

Fig 3

B

IR

Distance between somatic centers (μm)

A

B

A

23.1%

16.7%

Lateral

B

16.7%

27.0%

Dorsal

C

16.7%

200 μm

7.6%

Anterior

Fig 4

A

Original Volume
Original Shape

Average Volume
Original Shape

200 μm

B

27.3%

Lateral

20.4%

C

20.4%

Dorsal

32.8%

D

20.4%

Anterior

200 μm

5.3%

Fig 5

A

Original Volume
Original Shape

Average Shape

Original Volume
Average Shape

200 μm

B

Lateral

29.6%

34.0%

C

Dorsal

34.0%

22.5%

D

Anterior

34.0%

200 μm

24.3%

Fig 6

Fig 8

A

B1 ML

IR

Distance between somatic centers (µm)

B2 DV

IR

Distance between somatic centers (µm)

B3 AP

IR

Distance between somatic centers (µm)

500 µm

C Average CHP shape

500 µm

Original Volume
Original Shape
Average Volume
Original Shape
Original Volume
Average Shape
Average Volume
Average Shape

p<0.05 OVOS vs AVOS
p<0.05 OVOS vs OVAS
p<0.05 AVOS vs OVAS

Fig 9

A

B1 ML

IR

Distance between somatic centers (µm)

B2 DV

IR

Distance between somatic centers (µm)

C Average CHP shape

500 µm

B3 AP

IR

Original Volume Original Shape
Average Volume Original Shape
Original Volume Average Shape
Average Volume Average Shape

p<0.05 OVOS vs AVOS
p<0.05 OVOS vs OVAS
p<0.05 AVOS vs OVAS

500 µm

Distance between somatic centers (µm)

Fig 10

Fig 11