

1 **Rapid detection of *Staphylococcus aureus* and *Streptococcus pneumoniae* by real-time analy-**
2 **sis of volatile metabolites**

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12 **Running title: Early detection of bacteria by SESI-HRMS**

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22 **ABSTRACT**

23 Rapid detection of pathogenic bacteria is needed for rapid diagnostics allowing adequate and
24 timely treatment. In this study, we aimed to evaluate the technical feasibility of Secondary Elec-
25 tro-Spray Ionization-High Resolution Mass Spectrometry (SESI-HRMS) as a diagnostic tool for
26 rapid detection of bacterial infections and compare its performance with the current standard of
27 diagnostics. We compared the time required to confirm growth of the pathogenic bacteria *Staphy-*
28 *lococcus aureus* and *Streptococcus pneumoniae* by conventional detection by culture and MAL-
29 DI-TOF vs. detection of specific volatile organic compounds (VOCs) produced by these human
30 pathobionts. SESI-HRMS could consistently detect VOCs produced by *S. aureus* or *S. pneu-*
31 *moniae* on blood agar plates within minutes, allowing to positively identify bacteria within hours.
32 Unique *S. aureus* and *S. pneumoniae* features were detected already at bacterial densities as low
33 as $\sim 10^3$ colony forming units. Rich mass spectral fingerprints allowed for the distinction of these
34 two bacteria on a species and even strain level. To give an incentive towards clinical application
35 of this technology, further analyzed 17 clinical samples previously diagnosed by conventional
36 methods. We predominantly obtained a separation of samples which showed growth (i.e. pres-
37 ence of living bacteria) compared to samples with no bacterial growth (i.e. presence of dead bac-
38 teria). We conclude that SESI-HRMS allows rapid identification of unique bacterial features.
39 Further development of real-time analysis of clinical samples by SESI-HRMS will shorten the
40 time required for microbiological diagnosis with a high level of confidence and sensitivity and
41 should help to improve patient's tailored treatment.

42 **IMPORTANCE**

43 A timely identification of a pathogenic bacteria causing the infection is of pivotal importance for
44 the initiation of an adequate antimicrobial therapy. In this regard, different technologies have

45 been developed with the aim to achieve a highly reliable, specific, and overall fast identification
46 of pathogenic bacteria. However, conventional diagnostic techniques still require long prepro-
47 cessing times (hours to days) to acquire enough biological material for an accurate identification
48 of the pathogen. Therefore, in this work, we aimed to further shorten the detection time of current
49 gold standards for microbiological diagnostics by providing a system capable of a fast, sensitive
50 and specific discrimination of different pathogenic bacteria. This system relies on the real-time
51 mass spectrometric detection of volatile organic compounds (VOCs) produced by a given organ-
52 ism during its growth, potentially leading to a significant shortening of the time required to obtain
53 a positive reliable diagnostic.

54 **Key words:** bacterial infections; clinical diagnostics; real-time mass spectrometry; SESI-HRMS;
55 *Staphylococcus aureus*; *Streptococcus pneumoniae*

56 INTRODUCTION

57 A prompt and accurate identification of the causative pathogens of a bacterial infection is essen-
58 tial for providing patients with adequate treatments to reduce mortality and to prevent antibiotic
59 resistance (1-4). Bacterial infections caused by the human pathogenic bacteria *Staphylococcus*
60 *aureus* and *Streptococcus pneumoniae* remain highly prevalent (5-8). Despite the development
61 and availability of antibiotics, mortality remains high, reaching 20 % for *S. aureus* associated
62 endocarditis and more than one million deaths of children below 5 years of age by *S. pneumoniae*
63 (5, 7).

64 Currently, state-of-the-art bacterial identification methods consist of different strategies: in addi-
65 tion to conventional growth based diagnostics, molecular methods (16S-rRNA, whole genome
66 sequencing and antigen detection) and Matrix Assisted Laser Desorption/Ionization-Time of
67 Flight (MALDI-TOF) mass spectrometry, are the current culture based gold standards for identi-

68 fication of bacteria (9-12). Both methods portray complementary properties. Molecular methods
69 allow for detection of single bacterial components such as pneumococcal antigen or DNA direct-
70 ly in a clinical sample. This translates into a similar diagnostic tool comparable to MALDI-TOF,
71 at the cost of not being able to differentiate between live and dead bacteria or to present limita-
72 tions to identify antibiotic susceptibilities (13). On the other hand, the rich peptide fingerprints
73 detected by MALDI-TOF, allow for a very high degree of specificity, covering a vast range of
74 pathogens. However, this gold-standard method still bears limitations. In order to be able to iden-
75 tify a bacterium, a minimum concentration of bacteria have to be grown for a defined time to
76 allow an accurate identification of the sample (9, 10, 14-16). Such prerequisite introduces addi-
77 tional time for diagnosis of approximately 16 to 24 hours until the bacteria have grown sufficient-
78 ly (17-19).

79 Additional experimental methods are being developed to overcome these limitations of the tech-
80 niques currently accepted in microbiological diagnostics. One such an approach is to detect vola-
81 tile metabolites (i.e. volatile organic compounds aka VOCs) released by microorganisms as they
82 grow (20, 21). By doing so, the limitations of molecular methods such as time to positive detec-
83 tion and distinguishing between dead and alive bacteria is overcome. In addition, similarly to the
84 specificity provided by the peptide profiles captured by MALDI-TOF, the unique metabolism
85 developed over millions of years of evolution of bacteria provides an opportunity to render a high
86 specificity. This strategy has been usually pursued by different mass spectrometric variants. The
87 workhorse of VOCs analysis released by bacteria has been gas chromatography-mass spectrome-
88 try (GC-MS), which allows detecting very complex gas mixtures (22). However, the method is
89 also cumbersome, as it requires lengthy sample preparation, limiting the possibilities of providing
90 quicker results than MALDI-TOF-based analyses. Alternative real-time mass-spectrometric tech-
91 niques such as selected ion flow tube-mass spectrometry (SIFT-MS) (23-26) and Secondary Elec-

92 tro-Spray Ionization-High Resolution Mass Spectrometry (SESI-HRMS) (27-37) can provide
93 analyses of VOCs on the fly, thus potentially shortening time-to-results.

94 Despite the encouraging results and evidence accumulated over decades of analysis of VOCs
95 released by pathogens, such analytical strategy did not make it to transition from a research level
96 to a commercially available solution. Some of the reasons include that it is unclear yet whether
97 the sensitivity of such methods is enough to detect bacterial growth during very early stages of
98 bacterial replication, hence potentially accelerating positive results to just a few hours. Another
99 remaining question is whether at such low VOCs concentration levels, the selectivity is enough to
100 enable species differentiation. In this work, we addressed these open questions using SESI-
101 HRMS, which features limits of detection for VOC features as low as a part-per-trillion (38). Addi-
102 tionally, SESI-HRMS allows for the simultaneous detection of hundreds of VOCs from microor-
103 ganisms because of the high resolution of the mass analyzer (39). To do so, we conducted quanti-
104 tative measurements of two different *S. aureus* and *S. pneumoniae* strains. Parallel image analysis
105 and gold-standard culture and MALDI-TOF measurements were used to benchmark the technol-
106 ogy. We culminated the study providing proof-of-principle on the feasibility of this sample prep-
107 aration-free approach to ‘sniff-out’ a variety of clinical samples.

108 **RESULTS**

109 **Sensitivity measurements: quantifying the detection limit of colony forming units (CFUs)**

110 To evaluate the sensitivity of SESI-HRMS for the detection of bacterial VOC features, we meas-
111 ured a low number of CFUs (140 – 2000 CFUs per plate) of *S. aureus* and *S. pneumoniae* strains
112 over ~ 15 hours with SESI-HRMS. In parallel, time-lapse (TL) images were acquired to record
113 bacterial growth over 15 h and up to 38 h for certain replicates (Fig 1 and Fig S1). As an exam-
114 ple, figure 1A shows a representation of a time trace for a mass spectral feature observed in *S.*

115 *aureus* Cowan1 during SESI-HRMS measurement at a mass-to-charge ratio (m/z) 144.0476.
116 Complementary TL pixel intensities for each replicate are presented in figure 1B, accompanied
117 by control measurements together with TL image row examples at 15 h, 24 h and 38 h of meas-
118 urement. No bacteria were visually detected by the TL system by the end of SESI-HRMS acqui-
119 sition at 15 h. In contrast, m/z 144.0476 in *S. aureus* Cowan1 was detected by SESI-HRMS in all
120 four replicates within the first minutes of growth/measurement even if CFU numbers are as low
121 as 140 CFUs (Fig 1A). To control for bacterial growth, the plates were further analyzed for time
122 lapse beyond the 15 h analysis with SESI-HRMS, confirming the appearance of colonies after 24
123 h of growth (Fig 1B). In general, growth was detected for all bacterial strains under low CFU
124 condition as well as under high CFU condition (Fig S1).

125 **Selectivity measurements: Real-time detection of unique features on species and strain level**

126 After confirming the detection of features under a low number of CFUs, we investigated whether
127 these detected features were attributable to the *S. aureus* strains JE2 and Cowan1 or the *S. pneu-*
128 *moniae* strains D39 and TIGR4. We were able to assign a total of 392 features to the two bacteri-
129 al species or their respective strains as summarized in table S1. We found that out of 392 features,
130 51 features were *S. aureus*-specific (JE2 and Cowan1), 302 features were unique to *S. aureus* JE2
131 and 15 features unique to *S. aureus* Cowan1. Moreover, 18 features were identified as *S. pneu-*
132 *moniae*-specific (D39 and TIGR4), five features were unique to *S. pneumoniae* D39 and one fea-
133 ture was unique to *S. pneumoniae* TIGR4.

134 Since the features listed in table S1 identified for low CFUs (in the order of thousands) were not
135 always present in all biological replicates, we aimed to evaluate the use of SESI-HRMS with high
136 – density (billions) CFUs cultures to increase the signal strength and achieve a better reproduci-
137 bility among the biological replicates. Table S2 summarizes the total of 1,269 features detected

138 under high density conditions. Out of the total of 1,269 features, 19 features were detected in both
139 *S. aureus* strains JE2 and Cowan1. Three specific features were only found in *S. aureus* Cowan1
140 and 26 features in *S. aureus* JE2. For *S. pneumoniae*, 15 specific features were present in both
141 strains D39 and TIGR4. When both *S. pneumoniae* strains were evaluated separately, 1,206 fea-
142 tures were unique to *S. pneumoniae* D39 and no unique features were identified for TIGR4.

143 Out of the 26 features assigned to the strain *S. aureus* JE2, one representative feature at m/z
144 104.1069 is shown for all biological replicates and the controls (Fig 2A). The signal of this par-
145 ticular feature was more abundant in all four *S. aureus* JE2 replicates with a signal intensity of \sim
146 4×10^5 (a.u.) and nearly absent among all other strains and controls (Fig 2A). A similar profile was
147 shown for additional nine features depicted in the heat maps of *S. aureus* JE2 (Fig 2A). They start
148 to be detectable at \sim 5 h with increasing abundance towards the end of the measurement at 15 h.
149 In contrast, the features remained at the baseline level for the rest of strains and for the control.
150 Another example of *S. aureus* species specific time profiles is shown in figure 2B. Out of 19 fea-
151 tures detected in both *S. aureus* strains JE2 and Cowan1, a relevant feature at m/z 101.0608 is
152 shown for all biological replicates and controls (Fig 2B). Very similar to figure 2A, this particular
153 feature started to increase towards the end of the measurement and was only present in both *S.*
154 *aureus* strains with a high signal intensity and nearly not detected in the other strains and con-
155 trols. Figure S2 shows the heatmaps and/or representative specific features identified for the re-
156 maining species and strains. Unique features were assigned to each strain and species with the
157 exception of *S. pneumoniae* TIGR4 for which no unique features were assigned, albeit its growth
158 was confirmed by TL (Fig S1). Nevertheless, some features were present in *S. pneumoniae*
159 TIGR4 whereas they were absent in the control (Fig S2E).

160 Furthermore, we also compared the overlap of features detected using low density culture (Table
161 S1) versus using a high-saturated growth plate (Table S2). Only six species *S. pneumoniae* spe-
162 cific features were found under both conditions (Fig S3).

163 **Diverging metabolic trajectories of bacterial strains**

164 Next, we investigated the evolution over time of the features produced by the different bacteria
165 under investigation as they grew. Given the large number of features detected, we visualized our
166 multivariate dataset using Principal Component Analysis (PCA) and dendrogram trees to obtain
167 clusters of the different bacterial strains at different stages of bacterial growth (Fig 3, Fig S4 and
168 Fig S5). An initial separation of *S. pneumoniae* D39 from the other strains became apparent after
169 15 min of measurement (Fig S4). At the time point 7 h, a separation was noted for the *S. aureus*
170 JE2 replicates. The *S. aureus* Cowan1 group started to drift apart from the controls at 10 h after
171 growth. The best discrimination of the different groups was observed at 12 h as shown in the
172 PCA and dendrogram tree in figure 3. Except of *S. pneumoniae* TIGR4, all strains could be dis-
173 tinguished from the controls very clearly. Furthermore, it is well visible how Euclidean distance
174 shortens as a function of growth time (Fig S5).

175 **Measurement of clinical patient samples by SESI-HRMS**

176 After assessing the quantitative and qualitative capabilities of our real-time analysis system to
177 detect bacterial growth in enriched bacterial cultures, we tested the feasibility of such an ap-
178 proach for the direct analysis of a heterogeneous set of 17 clinical samples from 13 different pa-
179 tients derived from various origins including heart valves, skin, deep tissue, as well as foreign
180 bodies such as pacemakers (Table 1). All clinical samples were initially analyzed by routine di-
181 agnostics and the etiological agents identified by MALDI-TOF. Most samples came from patients
182 which underwent antibiotic therapy prior to SESI-HRMS measurement. Hence, for 10 out of the

183 17 clinical samples, no bacterial growth was detected by conventional growth on agar plates. For
184 the remaining seven samples for which bacterial growth was detected, four were *S. aureus* posi-
185 tive and three grew *S. epidermidis* at the time of measurement by SESI-HRMS (Table 1). This is
186 a typical problem encountered in clinics rendering the current culture based microbiological di-
187 agnostics inefficient. Indeed, our clinical information confirmed that 11 out of 13 patients from
188 this study were previously treated with different doses of antibiotics, and no bacterial growth
189 could be detected at the sampling time for eight out of 13 of these patients (Table 1).

190 Despite these challenges, all samples obtained from patients were subjected to a targeted analysis
191 whereby the specific features previously identified under high-density conditions were extracted
192 from the clinical dataset. To then visualize this highly complex dataset, t-SNE analysis was per-
193 formed (Fig 4). A clear cluster in the middle of the t-SNE space consisting of clinical samples
194 from *S. aureus* (methicillin-susceptible, MSSA) and *S. epidermidis* infections are visible. For
195 these samples, growth of bacteria was confirmed *a posteriori* (Table 1). In addition, two clinical
196 *S. aureus* samples (MRSA, further growth not confirmed) clustered at the bottom-right of the t-
197 SNE space.

198 **DISCUSSION**

199 In this study we showed that SESI-HRMS detects in real-time unique features of the human path-
200 ogens *S. aureus* and *S. pneumoniae* within minutes of growth on an agar plate and of distinct
201 strains. A high level of sensitivity for cultures with less than 1000 CFUs was achieved with de-
202 tectable features, allowing for a clear differentiation between these important two human bacteri-
203 al pathogens, even within strains. Since bacterial numbers are often low in patient samples, espe-
204 cially if the patients already is undergoing antimicrobial therapy, this is of great importance for
205 future diagnostics.

206 For any diagnostic method to be of clinical use, it requires to be sensitive and specific enough to
207 enable meaningful further clinical decisions such as an accurate antibiotic treatment. A third di-
208 mension of crucial importance in diagnostics of suspected bacterial infection is time-to-response.
209 A perfect diagnostic method should be sensitive enough to detect a positive sample during early
210 phases of infection, selective enough to distinguish different species or strains and should be fast
211 and require little-to-no sample preparation. Currently, state-of-the-art DNA-based diagnostic
212 methods for bacterial identification require just a single bacterial component to provide a positive
213 response (18). However, limitations include that no differentiation between live and dead bacteria
214 or a limited identification of antibiotic susceptibilities are possible. These limitations can serious-
215 ly affect its clinical usefulness (10). On the other side, peptide profile identification by mass spec-
216 trometric methods can overcome these two noted limitations of DNA-based methods. However,
217 this comes at the expense of requiring relatively lengthy pre-growing steps to enable active and
218 sufficient bacterial cells to be detected by the MALDI-TOF system (17, 40, 41).

219 The proposed mass spectrometric method lies somewhere in between these two techniques, hence
220 overcoming some of their limitations. On the one hand, detectable features accumulate in the
221 headspace of the specimen only if the bacteria replicate, hence are alive. On the other hand, the
222 data presented in here regarding the sensitivity of the SESI-HRMS suggests that bacterial loads in
223 the order of 10^3 CFUs are enough to be detected within one hour, well before sophisticated image
224 analysis methods detect any indication of macroscopic bacterial growth which is the current gold
225 standard in diagnostics. Also importantly, the proposed approach analyzes features in real-time,
226 hence enables monitoring the blood agar plates directly as the bacteria grow. This provides a
227 large automation potential as one can easily envisage multiplexing multiple dishes whereby an
228 automatic valve would switch across samples to monitor their growth every few minutes.

229 Regarding the selectivity required to discriminate different pathogens, the high resolution of Or-
230 bitrap mass analyzers enables the separation of typically thousands of ions in the m/z range of 50-
231 500, where most of the features from VOCs lie (42). Such resolving power renders a very high
232 specificity potential when it comes to distinguish specific metabolic patterns stemming from dif-
233 ferent microorganisms. In our case, hundreds of features were found to be specific for each spe-
234 cies. For the first time, we showed here that such level of specificity can go down to the strain
235 level, reinforcing the notion that metabolomics is very well suited to capture such subtle hetero-
236 geneity as it provides a downstream read-out of genetic plus environmental factors (43, 44). The
237 different environments between low- and high- CFU conditions may well explain the rather di-
238 verse metabolic signature observed under both conditions, leading to a modest overlap in the fea-
239 tures detected under such different conditions.

240 Thus, overall SESI-HRMS identification of bacterial species by the present design suggests a
241 high level of sensitivity and specificity, whereby already after 6 minutes, some strains, like *S.*
242 *pneumoniae* D39, differ substantially from negative controls. The best separation was observed
243 after 12 hours, which can be significantly quicker than the current MALDI-TOF identification
244 procedures.

245 Proof-of-principle of the applicability of the method in a more realistic clinical context was also
246 achieved by measuring clinical samples, including patient tissue and foreign material (e.g. pace-
247 makers). This is one key advantage of this technique, as it requires no sample preparation, and
248 therefore it is suitable for any solid or liquid specimen with a total analysis time of five-ten
249 minutes to fingerprint the samples. In this study, 17 clinical samples from different origin were
250 measured by SESI-HRMS. Following the standard procedure after a bacterial infection is diag-
251 nosed, those patients received antibiotics aiming to clear the infection. This often interferes with

252 diagnostics because bacteria do not grow anymore after antibiotic challenge as was the case at the
253 time of sampling and analysis by SESI-HRMS.

254 Four out of seven samples with an ongoing *S. aureus* infection and positive bacterial growth at
255 the time of the analysis, clustered together in the t-SNE space (Fig 4). These results were ob-
256 tained despite a low bacterial load in the clinical samples. While these results should be interpret-
257 ed with caution, they clearly suggest that the proposed methodology for diagnostics in bacterial
258 infections can be used with unprocessed clinical material. Similar to the peptide libraries used in
259 MALDI-TOF bacterial analysis, further clinical work should be devoted to construct mass spec-
260 tral libraries of VOCs, combined with modern classification algorithms to enable this technology
261 and complement current state-of-the-art diagnostics.

262 This study also comes with limitations that need to be addressed, such as the use of only Gram-
263 positive bacteria. In addition, this study didn't evaluate the identification of *Streptococcus mitis*
264 or other difficult to identify bacteria. However, given the ability of this technique to identify
265 unique features between two different strains of the same species, we believe this approach will
266 allow for a more accurate determination of difficult-to-identify bacteria. Additionally, a machine-
267 learning algorithm will need to be constructed using a much larger library of bacteria species and
268 strains in a follow up study to validate our findings at a much larger scale including both Gram-
269 positive and Gram-negative bacteria of clinical interest.

270

271 **CONCLUSIONS**

272 In this study, we tested the concept of exploiting the fact that bacteria produce complex volatile
273 metabolic mixtures as they proliferate. SESI-HRMS features a high gas-phase species' sensitivi-
274 ty, a great selectivity driven by the high-resolution of the mass analyzer. This was accomplished

275 in real-time, without any sample preparation. These characteristics allowed for the first time to
276 monitor the kinetic profiles of hundreds of metabolic species emitted by *S. aureus* and *S. pneu-*
277 *moniae* as they grew on agar plates. These hundreds of features rendered highly specific signa-
278 tures, which enabled distinguishing the samples even at the strain level. Finally, we scaled-up the
279 concept to test the feasibility of evaluating clinical samples retrieved from patients with bacterial
280 infections. The results showed that such samples can be fingerprinted within five minutes. Char-
281 acteristic metabolic patterns emerged, suggesting the potential of such an approach to comple-
282 ment current diagnostic methods. Further studies are required to construct VOC libraries of such
283 specimens retrieved from patients to further test the clinical utility of this method.

284 **MATERIALS AND METHODS**

285 **Bacterial Growth**

286 *S. aureus* (JE2 and Cowan1) and *S. pneumoniae* (D39 and TIGR4) were initially cultivated axen-
287 ically from glycerol stocks on Columbia agar plates with 5% sheep blood (BioMérieux) at 37°C
288 and 5% CO₂ for ~15 to 16 hours (Fig 5A). Two different sets of experiments were performed
289 with each strain. The first experiment consisted of plating a high-density culture (i.e. high CFUs)
290 by performing a subculture on a fresh blood agar plate directly from the overnight plate. In the
291 second experiment, the initial overnight culture in agar was resuspended in PBS and diluted to
292 obtain a low number of CFUs (i.e. low CFUs) ranging from ~140 to ~2000 CFUs per plate.

293

294 **Sampling of Clinical Patient Material**

295 Clinical samples were obtained from patients with bacterial infections requiring surgery. The
296 description of the different clinical samples used in this study such as origin, identified bacterial

297 pathogen, and antibiotic treatment prior to sampling is depicted in table 1. The processing of the
298 patient material depended on the characteristics of the sample. To verify the growth of bacteria
299 from these samples, the original sample was divided into two parts, one for measurement by SE-
300 SI-HRMS (Fig 5B) and one for colony plating and quantification. In short, samples such as skin,
301 heart valves and soft tissues were processed by disrupting the tissue using a tissue lyser (Qiagen
302 TissueLyzer, vibration frequency of 30/s for 10 minutes). For foreign material such as pacemak-
303 ers, the processing involved an initial sonication step of 5 minutes using a sonicator bath (Ultra-
304 sonic bath XUBA3, Grant) in sterile PBS. Following these two initial steps, the remaining pro-
305 cessing protocol was the same for all samples. The resulting suspension was washed twice with
306 sterile PBS to remove traces of antibiotics from the sample and a final step with sterile milliQ
307 water was used to lyse the eukaryotic cells. The sample was then serial diluted in sterile milliQ
308 water, plated on blood agar plate and incubated at 37 °C. In total, 17 clinical samples were used
309 for analysis.

310 **Sample Measurement with SESI-HRMS**

311 The experimental set-up consisted of a custom-made plexiglass box with an airtight closing
312 mechanism which was directly connected to an ion source (Super SESI, FIT, Spain) coupled to a
313 high-resolution mass spectrometer (Exactive Plus, Thermo Fisher Scientific, Germany) (Fig 5B).
314 The sample (bacteria plate or clinical patient material) was placed inside the plexiglass box which
315 was heated at 37 °C in a water bath. A mass flow controller was coupled to the box on the oppo-
316 site side of the SESI-HRMS via PTFE - tubes and ensured a constant medical grade air supply
317 through the system at a flow rate of 0.5 L/min and carried the VOCs emitted by the bacterial cul-
318 tures or from the clinical material towards the SESI-HRMS. Mass spectral analysis of bacteria
319 plates was conducted over a period of ~15 hours and for 5 min in case of clinical samples. An

320 automated switch system (Auto Click Typer version 2.0) allowed to alter between positive and
321 negative ionization mode every 30 minutes when measurements were conducted for ~15h. In
322 addition, a high-resolution camera was placed above the box and was triggered as described in
323 the “bacterial plate imaging” section of the methods. In total, 36 measurements were performed
324 whereby for both conditions (high-density and low CFUs) a total of 16 measurements were con-
325 ducted each (n=4 biological replicates per strain) along with measurements of empty blood agar
326 plates which served as control measures (n=4) for both CFU conditions.

327 To generate the electrospray in the SESI, a 20- μ m ID TaperTip silica capillary emitter (New Ob-
328 jective, USA) and a solution of 0.1% formic acid in water were used. The pressure of the SESI
329 solvent environment was set to 1.3 bar. Temperature of the ionization chamber and the sampling
330 line was set to 90 °C and 130 °C respectively. The voltage of the electrospray was set to 3.7 KV
331 in positive and 3 KV in negative ionization mode. The sheath gas flow rate was set to 10, capil-
332 lary temperature was 320 °C and S-lens RF level 50.0.

333 Mass spectra were acquired via Thermo Exactive Plus Tune software (version 2.9) in full scan
334 mode (scan range 50 – 500 m/z , polarity positive or negative, microscan number 10, ACG target
335 10^6 , maximum injection time 50 ms) at a resolving power of 140000 at m/z 200. The system was
336 calibrated on a regular basis before the measurements externally and internally by using common
337 background contaminants as lock masses in the respective polarity (45, 46).

338 **Bacterial Plate Imaging**

339 Simultaneously as the plate was analyzed for the production of VOCs by SESI-HRMS, a Time
340 lapse (TL) imaging experiment was performed using a high-resolution camera (Canon EOS
341 1200D reflex) triggered every 10 minutes by an Arduino Uno board (Arduino) to capture images

342 of the plate inside the box to visually document bacterial growth (47). To verify the growth of the
343 bacteria on the plate, TL measurement was conducted until ~ 40 h for specific replicates.

344 **SESI-HRMS Data Analysis**

345 Data analysis was performed using MATLAB (version 2021b, MathWorks Inc., USA). Raw
346 mass spectra files were accessed via inhouse C# console apps based on Thermo Fisher Scien-
347 tific's RawFileReader (version 5.0.0.38). MATLAB functions, *mspeaks* and *ksdensity* were ap-
348 plied to extract the final list of features. As a result, a data matrix of total 571 x 3460 (files x mass
349 spectral features) in positive mode and x 1129 mass spectral features in negative mode was ob-
350 tained. Specific m/z peaks had to be excluded due noisy interferences from the mass spectrome-
351 ter. Signal intensity time traces of all features were then computed and smoothed (moving mean;
352 span = 300) for visualization purposes. The mean Area Under the Curve (mAUC) of the time
353 traces (n=4 replicates per strain) was calculated by interpolating the data every 0.01h. To identify
354 features, unique to a particular bacterial strain, two criteria were defined; first criteria kept only
355 features with a log₂ fold change (FC) ≥ 2 in mAUC of a particular strain compared to the mAUC
356 of the control and 2nd criteria required a log₂ FC ≥ 4 in mAUC of the particular strain compared to
357 the averaged mAUC of the other investigated strains. Furthermore, species specific time traces
358 were identified, meaning that they had to be present in both *S. pneumoniae* strains (D39 and
359 TIGR4) or both *S. aureus* strains (JE2 and Cowan1). Therefore three criteria were defined: first
360 criteria kept only features with a log₂ FC ≥ 2 in mAUC in both strains of a particular species
361 compared to the mAUC of the control; 2nd criteria defined to only consider the features further if
362 within one species the respective strains had at least a mAUC of 30% of the mAUC of the other
363 strain under the respective species to avoid features to be selected which tended to be rather pre-
364 sent in one strain and not in both; 3rd criteria considered only features which showed a log₂ FC \geq

365 4 in average mAUC of the two strains of one species compared to the average mAUC of the two
366 strains of the other species and vice versa. In a next step the time traces of features unique for the
367 different strains and species were auto scaled (z-score), subjected to a hierarchical cluster tree
368 (Ward method; Euclidean distance) and visualized as heat maps showing the evolution of the
369 features over time. Principal Component Analysis (PCA) of 5th – root transformed data matrix
370 and a hierarchical binary cluster tree (Ward Method; Euclidean distance) were used to visually
371 discriminate the different bacterial strains at distinctive time points over ~15 hours. Clinical sam-
372 ples were analyzed using a targeted approach, where unique positive and negative time traces of
373 features previously identified for the different strains under high density CFU condition were
374 directly extracted from the clinical samples raw data using in-house C# console app based on
375 RawFileReader which resulted in a data matrix of 17 x 1269 (samples x mass spectral features).
376 We then performed t-distributed stochastic neighbor embedding (t-SNE) to visualize this highly
377 complex and exploratory dataset. For all features, molecular formulae were assigned based on
378 accurate mass by using the “seven golden rules” (48), considering the elements C, H, N, O, P and
379 S and the adducts [M + H], [M - H₂O + H], [M + NH₄], [M - NH₃ + H], [M + Na] in positive
380 mode and [M - H], [M - Na], [M - H₂O - H], [M + NH₃ - H], [M - NH₄] in negative ionization
381 mode.

382 **Image Data Analysis**

383 Simultaneously to the SESI-HRMS measurement, bacterial growth on agar was verified and
384 quantified by TL imaging. The acquired TL images were analyzed with a custom extension for
385 ColTapp (47) to quantify the bacterial growth as changes in pixel intensity over time. As the vis-
386 ual growth pattern of *S. aureus* and *S. pneumoniae* are distinct, different image analysis pipelines
387 were utilized. For *S. aureus*, images were transformed to grayscale by selecting the green channel

388 of the RGB image and subsequent top-hat filtering was performed to reduce lighting heterogeneity.
389 ty. For *S. pneumoniae*, the RGB images were transformed to YIQ color space and subset to the I
390 channel only. A gaussian filter was applied to the first image of the TL series to define a back-
391 ground which then was subtracted from each other image in the TL series.

392 The following steps were the same for both species: the corrected grayscale images were subset
393 to include only the area within plate boundaries. Then, min-max scaling with [0, 0.7] as range
394 was applied to the pixel intensities. Finally, the sum of all pixel intensities was divided by the
395 sum of pixels to derive a normalized intensity value per time point of a TL image series.

396 **Ethical Statement**

397 For this study, samples from patients with vascular graft /endovascular infections, infective endo-
398 carditis, bone and prosthetic joint infections and any other infections were collected under the
399 framework of the Vascular Graft Cohort study (VASGRA; KEK-2012-0583), the Endovascular
400 and Cardiac Valve Infection Registry (ENVALVE; BASEC 2017-01140), the Prosthetic Joint
401 Infection Cohort (Balgrist, BASEC 2017-01458), and BacVivo (BASEC 2017-02225), respec-
402 tively. The study was approved by the local ethics committee of the Canton of Zurich, Switzer-
403 land

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416 **Author Contributions**

417 Conception and Design, AGM, KA, PS and ASZ; Clinical Sample Collection and Processing,
418 AGM, TCS, SDB and ASZ. Data Analysis and interpretation, AGM, KA, JB, KDS, PS and ASZ.
419 Manuscript Writing – Original Draft, AGM, KA, PS and ASZ. Writing, Review & Editing,
420 AGM, KA, JB, KDS, TCS, SDB, PS and ASZ. All authors read and approved the final manu-
421 script.

422 **Conflicts of interest**

423 PS is cofounder of Deep Breath Initiative A.G. (Switzerland), which develops breath-based diag-
424 nostic tools. KDS is consultant for Deep Breath Initiative A.G. (Switzerland).

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584 **TABLES**

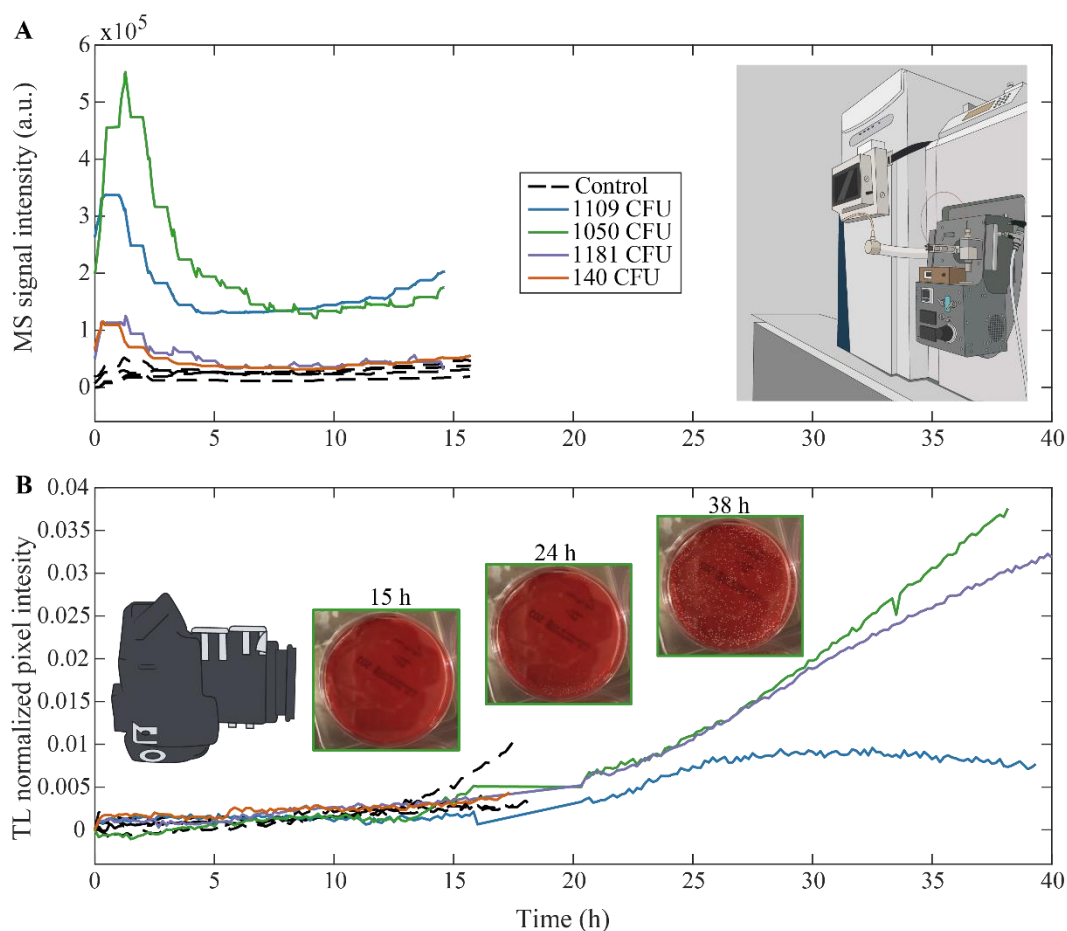
585 **Table 1** Clinical characteristics of patient samples analyzed by SESI-HRMS. Description of clin-
586 ical microbiology, detected growth by SESI-HRMS, sample type, clinical condition and whether
587 there was antibiotic treatment before analysis by SESI-HRMS.

<i>Sample identifier</i>	<i>Clinical Microbiology</i>	<i>Growth parallel to SESI-HRMS</i>	<i>Sample type</i>	<i>Condition</i>	<i>Antibiotics prior sampling</i>
1	Methicillin-resistant <i>Staphylococcus aureus</i> (MRSA)	no	Lung tissue	Pneumonia	yes
2	Methicillin-resistant <i>Staphylococcus aureus</i> (MRSA)	no	Blood	Bacteremia	not available
3	<i>Staphylococcus aureus</i> (MSSA)	no	Heart valve	Endocarditis	yes
4	<i>Staphylococcus aureus</i> (MSSA)	no	Heart valve	Endocarditis	yes
5	<i>Aggregatibacter</i> spp. <i>Actinomyces meyeri</i>	no	Lung tissue	Pneumonia with empyema	yes
6	<i>Staphylococcus aureus</i> (MSSA)	yes	Heart valve	Endocarditis	yes
7	<i>Staphylococcus aureus</i> (MSSA)	yes	Heart valve	Endocarditis	yes
8	<i>Staphylococcus aureus</i> (MSSA)	yes	Heart valve	Endocarditis	yes

9	<i>Staphylococcus aureus</i> (MSSA)	yes	Nasal aspirate	Bacterial sinusitis	yes
10	<i>Staphylococcus lugdunensis</i> <i>Staphylococcus epidermidis</i>	yes	Cardiac device	Pacemaker infection	no
11	<i>Staphylococcus epidermidis</i>	yes	Cardiac device	Pacemaker infection	no
12	<i>Staphylococcus epidermidis</i>	yes	Cardiac device	Pacemaker infection	no
13	not available	no	Cardiac device	Pacemaker infection	yes
14	<i>Staphylococcus aureus</i> (MSSA)	no	Cardiac device	Pacemaker infection	yes
15	<i>Streptococcus anginosus</i>	no	Cardiac device	Pleural empyema	no
16	<i>Parvimonas micra</i>	no	Lung tissue	Pleural empyema	yes
17	<i>Aggregatibacter (Haemophilus) aphrophilus</i>	no	Lung tissue	Thoracic hematoma	yes

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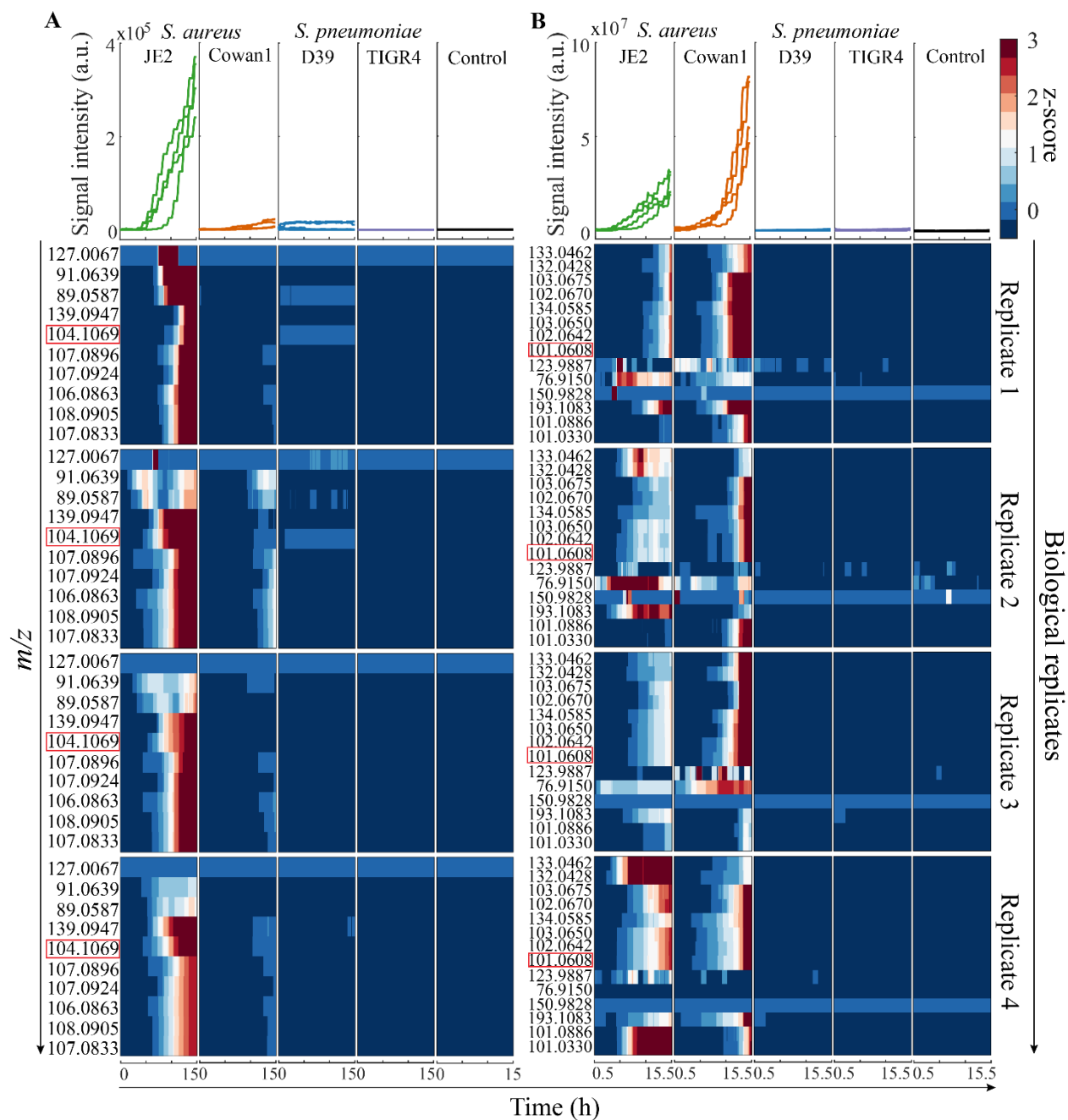
589 FIGURES



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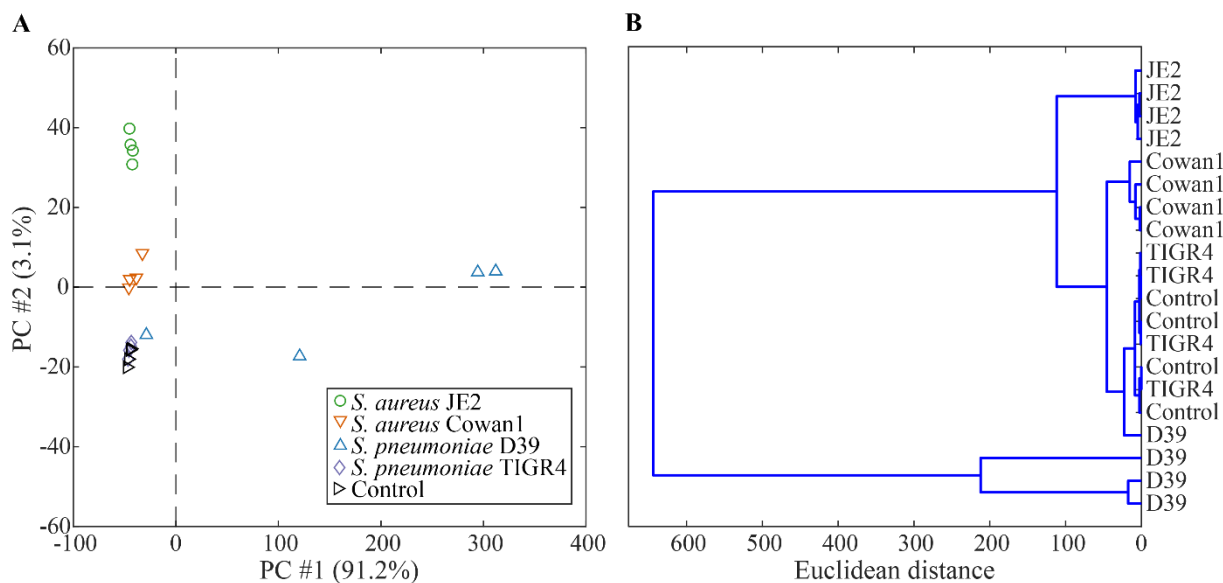
591 **FIG 1** Detection of features in headspace of growing bacterial culture by SESI-HRMS vs. visual
592 monitoring by TL camera. (A) Example of a feature time trace at m/z 144.0476 observed in *S.*
593 *aureus* Cowan1 by SESI-HRMS over 15 h of measurement. (B) Corresponding TL normalized
594 pixel intensity of the measured replicates along with pictures showing visually captured growth at
595 15 h, 24 h and 38 h after the bacteria were put on the plate. The four colored lines represent four
596 biological replicates and the four dashed black lines represent the four control replicates. The
597 colors indicate how many CFUs were put on the blood agar plate for each replicate measured.
598 MS=Mass spectrometer, CFU = Colony forming unit, TL = Time lapse.

599



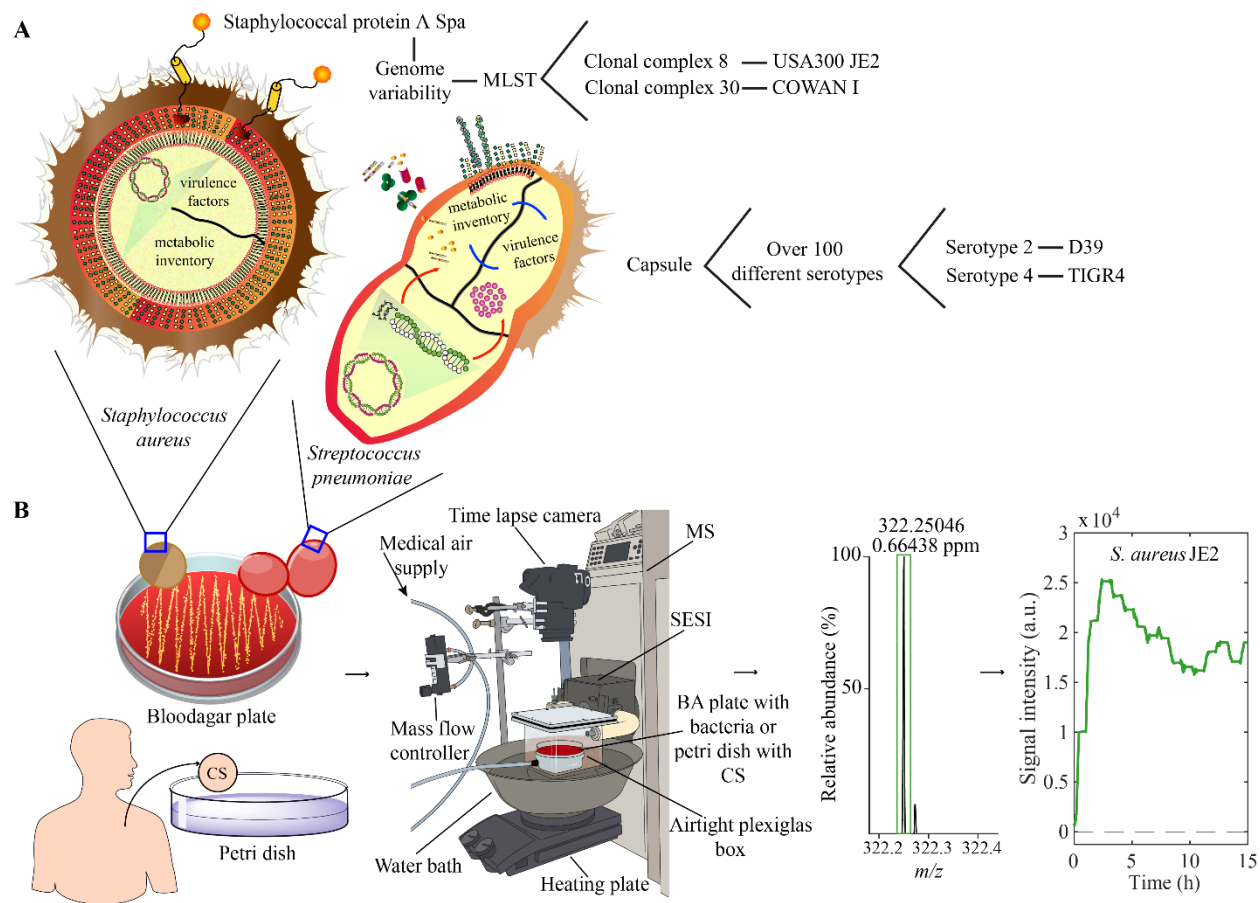
600
601 **FIG 2** Specific time – dependent features detected during bacterial growth. (A) Example time
602 trace of the positive ion at m/z 104.1069 (framed in red) unique to *S. aureus* JE2 is shown on top
603 of the heatmaps consisting of total ten features (positive ions) unique to *S. aureus* JE2. (B) Ex-
604 ample time trace of the negative ion at m/z 101.0608 (framed in red) unique to the species *S. au-*
605 *reus* (i.e. present in both JE2 and Cowan1) is shown on top of the heatmaps consisting of total 14

606 features (negative ions) unique to species *S. aureus*. Real-time evolution of all features is shown
607 over 15 hours of measurement by SESI-HRMS for all four investigated strains (n=4 biological
608 replicates) and controls (n=4). The color bar indicates the z-score values of absolute signal inten-
609 sity for each feature, from low (dark blue) to increased signal intensity (dark red).



611 **FIG 3** PCA score plot and dendrogram of PCA scores explaining 95% of variance illustrated at
612 time point 12 h after the start of measurement. (A) PCA score plot of 1235 strain specific features
613 (positive and negative ions) at 12 h identified for high CFU cultures. (B) Dendrogram showing
614 the detailed hierarchical relationship between bacterial species and strains at time point 12 hours.

615



624

625 **FIG 5** Experimental setup designed for the detection of features in the headspace of bacterial
 626 cultures by SESI-HRMS. (A) Genomic difference between the two species *S. aureus* and *S.*
 627 *pneumoniae* and their respective strains. (B) From left to right, either a strain of *S. aureus* (JE2 or
 628 Cowan1) or a strain of *S. pneumoniae* (D39 or TIGR4) on a blood agar plate or a clinical sample
 629 on a petri dish was placed in an airtight plexiglass box coupled to the SESI-HRMS. A TL camera
 630 was directly placed above the box for visualization of bacterial growth in parallel to the SESI-
 631 HRMS measurement. The setup ensured a closed environment where the features present in the
 632 headspace of the samples were guided through a medical grade air flow of 0.5 L/min towards the
 633 SESI where they were ionized and then separated according to their mass to charge ratio (m/z) in
 634 the MS, resulting in real-time traces over ~15 h (bacterial plates) and five minutes (clinical sam-

635 ples). BA = Blood agar, CS = Clinical sample, MS = Mass spectrometer, SESI = Secondary Elec-
636 tro-Spray Ionization.

637 **FIGURE LEGENDS SUPPLEMENTAL MATERIAL**

638 **FIG S1** TL of bacterial strains and blood agar controls under low and high CFU conditions. (A)
639 TL normalized pixel intensity of the control replicates. The control measures between the two
640 bacterial species (*S. aureus* and *S. pneumoniae*) looked different since a different analysis proto-
641 col was used for the evaluation. (B) TL normalized pixel intensity illustrated for the two *S.*
642 *pneumoniae* strains. (C) TL normalized pixel intensity illustrated for the two *S. aureus* strains.
643 The color legend represents the biological replicates (n=4) measured for each bacterial strain and
644 control along with the number of CFUs used under defined conditions for each biological repli-
645 cate. TL = Time lapse, CFU = Colony forming unit.

646 **FIG S2** Specific time – dependent features detected during bacterial growth. (A) Example time
647 trace of the positive ion at m/z 201.0433 unique to *S. pneumoniae* D39 is shown on top of the
648 heatmaps consisting of total 1178 features (positive ions) specific to *S. pneumoniae* D39. (B)
649 Example time trace of the negative ion at m/z 89.9913 unique to *S. pneumoniae* D39 is shown on
650 top of the heatmaps consisting of total 28 features (negative ions) specific to *S. pneumoniae* D39.
651 (C) Example time trace of the negative ion at m/z 209.1032 unique to *S. aureus* JE2 is shown on
652 top of the heatmaps consisting of total 16 features (negative ions) specific to *S. aureus* JE2. (D)
653 Example time trace of the positive ion at m/z 135.121 unique to *S. aureus* (JE2 and Cowan1) is
654 shown on top of the heatmaps consisting of total five m/z -features (positive ions) specific to *S.*
655 *aureus* (JE2 and Cowan1). (E) Example time trace of the negative ion at m/z 82.0298 unique to *S.*
656 *pneumoniae* (D39 and TIGR4) is shown on top of the heatmaps consisting of total 14 features
657 (negative ions) specific to *S. pneumoniae*. (F) Time trace of the only positive ion at m/z 235.0757

658 unique to *S. pneumoniae*. (G) Example time trace of the positive ion at m/z 179.1042 unique to *S.*
659 *aureus* Cowan1. Real-time evolution of all features is shown over 15 hours of measurement by
660 SESI-HRMS for all four investigated strains (n=4 biological replicates) and controls (n=4). The
661 color bar indicates the z-score values of absolute MS signal intensity for each feature, from low
662 (dark blue) to increased signal intensity (dark red).

663 **FIG S3** Overlapping features unique to *S. pneumoniae* (i.e. present in both D39 and TIGR4) un-
664 der low CFU and high CFU condition. (A) Venn diagram of overlapping features detected for
665 low and high CFU bacterial cultures. (B) Representative time trace of the positive ion at m/z
666 385.2214 observed in *S. pneumoniae* (D39 and TIGR4) for low and high-density cultures. CFU =
667 Colony forming unit.

668 **FIG S4** PCA score plots over time obtained for high density bacterial cultures. Score plots of
669 1190 strain specific features (positive ions) for time points 0.1 hour and 0.25 hour. Score plots of
670 1235 strain specific features (positive and negative ions) at distinct time points over the 15 hours
671 measurement period.

672 **FIG S5** Dendrogram trees over time obtained for high density bacterial cultures. Cluster analysis
673 of samples considering 1190 strain specific features (positive ions) for time points 0.1 hour and
674 0.25 hour. Cluster analysis of samples using 1235 strain specific features (positive and negative
675 ions) at distinct time points during the 15 hours measurement period.

676 **TABLE DESCRIPTIONS SUPPLEMENTAL MATERIAL**

677 **Table S1** Unique features assigned to *S. aureus* and *S. pneumoniae* in positive and negative ioni-
678 zation mode under low CFU condition.

679 **Table S2** Unique features assigned to the different strains of *S. aureus* and *S. pneumoniae* in pos-
680 itive and negative ionization mode under high CFU condition.

681