Analysis of calcium dynamics for dim-light responses in rod and cone photoreceptors

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Abstract

Rod and cone photoreceptors in the retina of vertebrate eyes are fundamental sensory neurons underlying vision. They use a sophisticated signal transduction pathway consisting of a series of biochemical processes to convert the absorption of light into an electrical current response. Several of these processes are modulated by feedback that depends on the intracellular Ca^{2+} concentration. In this work we use a representative phototransduction model to study how changing the Ca^{2+} kinetics by fast buffering affects sensitivity and dynamics of the light response in mouse rod and cone photoreceptors. We derive analytic results for dim-light stimulations that provide quantitative and conceptual insight. We show that flash responses are monophasic with low buffering, and the change in the Ca^{2+} concentration occurs in proportion to the current. If the amount of fast buffering is increased, the Ca^{2+} kinetics becomes slowed down and delayed with respect to the current, and biphasic responses emerge (damped oscillations). This shows that a biphasic response is not necessarily a manifestation of slow buffering reactions. A phase space analysis shows that the emergence of biphasic responses depends on the ratio between the effective rate μ_{ca} that controls the Ca^{2+} kinetics, and the dark turnover rate of cyclic GMP β_d. We further investigate how the light response is altered by modifying the extracellular Ca^{2+} concentration. In summary, we provide a comprehensive quantitative analysis that precisely links the dynamics of Ca^{2+} concentration to the observed current response.

1 Introduction

Vision in most vertebrates is sustained by rod and cone photoreceptors in the retina of the eyes [1]. Whereas rods are most sensitive to light and sustain vision in dim-light conditions, cones have a much reduced light sensitivity, but they adapt and thereby maintain vision even under brightest light conditions [2].

The signal transduction cascade in the outer segment of rod and cone photoreceptors is complex multistep process that transforms the absorption of light by photopigments into an electrical current (for reviews see [3, 4, 5, 6]). Many of these processes are modulated by Ca^{2+} feedback [7, 8, 9, 10, 11]. Ca^{2+} feedback not only controls how photoreceptors adapt to increasing light intensities [12, 13, 14, 15, 16], it also shapes the response in darkness [17, 18, 19, 20]. Dark adapted rods in most species show monophasic responses to brief flashes of light (monophasic means that the current is always reduced compared to its steady state level in darkness). If the Ca^{2+} kinetics is disturbed by the application of exogenous buffers, biphasic responses emerge (biphasic means that the current also reaches values that are larger than the steady state level). With exogenous Ca^{2+} buffers, biphasic flash responses have been observed in amphibian rods [21, 22, 20, 23, 24], in primate and guinea pig rods [25, 17, 14], and in mouse rods [17, 26]. In primate and mammalian cones, biphasic responses have often been observed even without exogenous buffer application [27, 28, 29, 30, 31, 32]. However, recently it has been claimed that cone responses are mostly monophasic under physiological conditions, and that

biphasic responses are most likely the result of a distorted negative Ca^{2+} feedback [33]. There it has also been shown that biphasic cone responses could be removed by lowering the extracellular Ca^{2+} concentration [33].

The dynamics of the free-Ca^{2+} concentration in the OS depends on influx through cyclic nucleotide-gated (CNG) channels, efflux via NCKX exchangers, and cytoplasmic buffering [6]. With negligible Ca^{2+} buffering, modelling shows that the Ca^{2+} concentration changes in proportion to the current, and flash responses are monophasic [34, 35]. Biphasic responses have been simulated with models that take into account the effect of buffering [36]. One possibility to model the effect of buffering is to consider explicit equations for the binding between free Ca^{2+} and the buffers [36, 37, 38, 39, 40, 41, 42]. A different approach, which is more frequently used, is to lump the effect of the various buffers into a single parameter called the buffering capacity B_{ca} [43, 44, 6, 45, 46, 47, 48, 49, 50] (a Ca^{2+}-dependent buffering capacity has been used in [27]). The use of a constant buffering capacity is a valid approximation if the binding kinetics are fast (fast buffers), and the Ca^{2+} affinity of the buffers is low compared to the physiological range of the Ca^{2+} concentration. Thus, whereas modelling of the binding reactions between Ca^{2+} and buffers is most accurate, models with a buffering capacity are an approximation, but simpler to handle.

So far, insight from modelling about the Ca^{2+} dynamics and the effect of buffering has been obtained almost exclusively from numerical simulations (but see the analysis in [43, 30, 44, 28]). Recently, we derived analytic results for the entire dim-light response that provided new insight about how the various biophysical processes determine amplitude and shape of flash responses in rods and cones [34, 35]. In this previous work, we neglected the effect of buffering, and assumed that the free-Ca^{2+} concentration changes in proportion to the current, which often is the physiological case [51, 19]. In the present manuscript, we generalize our previous analysis by studying how the dim-light response is modified if the Ca^{2+} dynamics becomes gradually delayed with respect to the current due to buffers with fast binding kinetics. We derive analytic formulas that reproduce a dim-light response in presence of buffering, which we use to obtain quantitative and conceptual insight. We show that biphasic responses (damped oscillations) emerge as the Ca^{2+} dynamics is slowed down. We study the phase space that separates monophasic from biphasic responses, and we determine how sensitivity and shape of responses are affected by buffering. Finally, we examine the impact of changing the extracellular Ca^{2+} concentration.

2 Materials and Methods

2.1 Phototransduction model

We start from the parsimonious phototransduction model introduced in [35, 34], and we include a more general Ca^{2+} dynamics where the free-Ca^{2+} concentration does not necessarily change in proportion to the circulating current. In short, light activates the visual pigment R^* with a rate that is proportional to the light intensity $\phi(t)$ times the collecting area κ. R^* activates the G-protein transducin T^* with a rate k_{act}, and deactivates with rate μ_{rh}. T^* activates phosphodiesterase (PDE) P^* with a rate k_{tr}, and deactivates with rate mu_{tr}. Because the deactivation of T^* is linked to the activation of PDE, we have $k_{tr} = \mu_{tr}$ (to keep the analysis most general, we distinguish between k_{tr} and μ_{tr}). P^* deactivates with rate μ_{pde}, and hydrolyses the cytosolic second messenger cyclic GMP (cGMP) with rate constant β_{sub}. cGMP gates the opening of CNG channels, in the OS membrane. The rate α by which the cGMP concentration c_{cg} is synthesized by guanylate cyclase (GC) depends on the free-Ca^{2+} concentration c_{ca}, $\alpha(c_{ca}) = \alpha_{max} \frac{r_\alpha c_{ca}^{n_\alpha} + K_\alpha^{n_\alpha}}{c_{ca}^{n_\alpha} + K_\alpha^{n_\alpha}}$, where $r_\alpha = \frac{\alpha_{min}}{\alpha_{max}}$. The cyclase activity is modulated via the intermediate binding of Ca^{2+} to GCAP proteins [52, 17]. Ca^{2+} also affects

the phosphorylation dependent deactivation of the photopigment by binding to recoverin, which inhibits the photopgiment phosphorylation by rhodopsin kinase [53, 54]. However, in this work we only consider the Ca^{2+} feedback to guanylate cyclase, which is most important under dim light conditions [17, 18, 19].

The Ca^{2+} concentration in the OS changes due to influx via CNG channels, and efflux via electrogenic NCKX exchangers. The CNG current is $I_{ch} = I_{ch,max}p_{ch}$, where $p_{ch} = \frac{c_{cg}^{n_{ch}}}{c_{cg}^{n_{ch}} + K_{ch}^{n_{ch}}}$ is the cGMP dependent fraction of open channels, and K_{ch} is the $cGMP$ concentration where 50% of the channels are open. Only the fraction $f_{ch,ca}$ of the CNG current is carried by Ca^{2+}, $I_{ch,ca} = f_{ch,ca}I_{ch}$. The influx of Ca^{2+} via CNG channels therefore is $\frac{I_{ch,ca}}{2e^+}$. The exchanger current as a function of the Ca^{2+} concentration is $I_{ex} = I_{ex,sat}p_{ex}$, where $I_{ex,sat}$ is the saturating current at high c_{ca}, and $p_{ex} = \frac{c_{ca}}{c_{ca}+K_{ex}}$ is the saturation level of the exchangers. The exchanger stoichiometry is such that the extrusion of a single Ca^{2+} leads to the influx of a single positive charge e^+, such that I_{ex}/e^+ gives the Ca^{2+} efflux.

Ca^{2+} binds to and regulates the activity of many proteins participating in the signal transduction cascade [15, 9, 10, 11]. In principle, all these reactions contribute to Ca^{2+} buffering. With N_b buffer species b_i ($i = 1, \ldots N_b$), the Ca^{2+} dynamics in the OS is governed by the equations

$$
\begin{aligned}
F_A V_{os} \frac{d}{dt}\left(c_{ca} + \sum_{i=1}^{N_b} c_{ca,b_i}\right) &= \frac{I_{ch,ca}}{2} - I_{ex} \\
\frac{d}{dt}c_{ca,b_i} &= \mu_{b_i}\left(\frac{(c_{b_i} - c_{ca,b_i})c_{ca}}{K_{b_i}} - c_{ca,b_i}\right), \; i = 1, \ldots N_b,
\end{aligned}
\tag{1}
$$

where c_{ca,b_i} are the Ca^{2+} concentrations that are bound to the buffer species b_i, c_{b_i} are total buffer concentrations, K_{b_i} are dissociation constants, μ_{b_i} are dissociation rates, $F_A = 9.65 \times 10^{-5} \frac{spA}{\mu M \mu m^3}$ is the Faraday constant, and V_{os} is the outer segment volume. In this work we restrict the analysis to buffering reactions that proceed much faster compared to the time scale of the current change. With fast buffering (large μ_{b_i}), $c_{ca,b_i}(t)$ becomes a function of the free-Ca^{2+} concentration $c_{ca}(t)$, $c_{ca,b_i}(t) \approx c_{b_i}\frac{c_{ca}(t)}{c_{ca}(t)+K_{b_i}}$ (quasi steady-state approximation). With fast buffers, Eq. 1 simplifies to

$$
F_A V_{os}\left(1 + \sum_{i=1}^{N_b}\frac{c_{b_i}K_{b_i}}{(c_{ca} + K_{b_i})^2}\right)\frac{d}{dt}c_{ca} = \frac{I_{ch,ca}}{2} - I_{ex}.
\tag{2}
$$

The complete system of transduction equations reads

$$
\begin{aligned}
\frac{d}{dt}R^* &= \phi(t)\kappa - \mu_{rh}R^* \\
\frac{d}{dt}T^* &= k_{act}R^* - \mu_{tr}T^* \\
\frac{d}{dt}P^* &= k_{tr}T^* - \mu_{pde}P^* \\
\frac{d}{dt}c_{cg} &= \alpha_{max}\frac{r_\alpha c_{ca}^{n_\alpha} + K_\alpha^{n_\alpha}}{c_{ca}^{n_\alpha} + K_\alpha^{n_\alpha}} - (\beta_d + \beta_{sub}P^*)c_{cg} \\
\frac{d}{dt}c_{ca} &= \frac{1}{F_A V_{os}}\left(1 + \sum_{i=1}^{N_b}\frac{c_{b_i}K_{b_i}}{(c_{ca} + K_{b_i})^2}\right)^{-1}\left(\frac{I_{ch,ca}(c_{cg})}{2} - I_{ex}(c_{ca})\right),
\end{aligned}
\tag{3}
$$

where β_d is the basal cGMP hydrolysis rate in darkness. The total current is

$$
I = I_{ch}(c_{cg}) + I_{ex}(c_{ca}) = I_{ch,max}\frac{c_{cg}^{n_{ch}}}{c_{cg}^{n_{ch}} + K_{ch}^{n_{ch}}} + I_{ex,sat}\frac{c_{ca}}{c_{ca} + K_{ex}}.
\tag{4}
$$

Next we use the concentrations $c_{ca,0}$ and $c_{cg,0}$, and the current I_0 to introduce normalized variables and parameters. Since we are interested in the light response in darkness, we choose $c_{ca,0}$, $c_{cg,0}$, and I_0 to be steady state values in darkness. These values can either be computed from Eq. 3 with $\phi(t) = 0$, or one can directly use the experimentally measured values for $c_{ca,0}$, $c_{cg,0}$ and I_0. In the latter case, we implicitly replaces the parameters α_{max}, $I_{ch,max}$ and $I_{ex,sat}$ (which are not well known) with $c_{ca,0}$, $c_{cg,0}$ and I_0. We introduce the normalized variable and parameters $\hat{c}_{cg} = \frac{c_{cg}}{c_{cg,0}}$, $\hat{c}_{ca} = \frac{c_{ca}}{c_{ca,0}}$, $\hat{c}_{b_i} = \frac{c_{b_i}}{c_{ca,0}}$, $\hat{K}_{ch} = \frac{K_{ch}}{c_{cg,0}}$, $\hat{K}_{ex} = \frac{K_{ex}}{c_{ca,0}}$, $\hat{K}_{\alpha} = \frac{K_{\alpha}}{c_{ca,0}}$, $\hat{K}_{b_i} = \frac{K_{b_i}}{c_{ca,0}}$, and we define the dark buffering constants $B_{ca,b_i} = \frac{c_{b_i} K_{b_i}}{(c_{ca,0}+K_{b_i})^2}$, such that $\sum_{i=1}^{N_b} \frac{c_{b_i} K_{b_i}}{(c_{ca}(t)+K_{b_i})^2} = \sum_{i=1}^{N_b} B_{ca,b_i} \frac{1+\hat{K}_{b_i})^2}{(\hat{c}_{ca}(t)+\hat{K}_{b_i})^2}$. Because $c_{ca,0}$ and $c_{cg,0}$ are steady state values, we have $\alpha(c_{ca,0}) = \beta_d c_{cg,0}$ and $I_{ch,ca}(c_{cg,0}) = f_{ch,ca} I_{ch}(c_{cg,0}) = 2 I_{ex}(c_{ca,0})$. To simplify the analysis, we further introduce $\tilde{P}^* = \beta_{sub} P^*$, $\tilde{T}^* = \frac{\beta_{sub} k_{tr}}{\mu_{pde}} T^*$, $\tilde{R}^* = \frac{\beta_{sub} k_{act} k_{tr}}{\mu_{pde} \mu_{tr}} R^*$, and the gain $\xi = \frac{k_{act} \beta_{sub} k_{tr}}{\mu_{rh} \mu_{pde} \mu_{tr}}$ [35]. With the steady state condition $\alpha(c_{ca,0}) = \beta_d c_{cg,0}$ we obtain from Eq. 3

$$
\begin{aligned}
\frac{d}{dt}\tilde{R}^* &= \mu_{rh}(\phi(t)\kappa\xi - \tilde{R}^*) \\
\frac{d}{dt}\tilde{T}^* &= \mu_{tr}(\tilde{R}^* - \tilde{T}^*) \\
\frac{d}{dt}\tilde{P}^* &= \mu_{pde}(\tilde{T}^* - \tilde{P}^*) \\
\frac{d}{dt}\hat{c}_{cg} &= \beta_d \hat{\alpha}(\hat{c}_{ca}) - (\beta_d + \tilde{P}^*)\hat{c}_{cg} \\
\frac{d}{dt}\hat{c}_{ca} &= \frac{1 + B_{ca}}{1 + \sum_{i=1}^{N_b} B_{ca,b_i} \frac{(1+\hat{K}_{b_i})^2}{(\hat{c}_{ca}+\hat{K}_{b_i})^2}} \mu_{ca}\left(\hat{p}_{ch}(\hat{c}_{cg}) - \hat{p}_{ex}(\hat{c}_{ca})\right)
\end{aligned}
\tag{5}
$$

with

$$
\begin{aligned}
B_{ca} &= \sum_{i=1}^{N_b} B_{ca,b_i} = \sum_{i=1}^{N_b} \frac{\hat{c}_{b_i} \hat{K}_{b_i}}{(1+\hat{K}_{b_i})^2} \\
\mu_{ca} &= \frac{1}{(1+B_{ca}) F_A V_{os}} \frac{I_{ex}(c_{ca,0})}{c_{ca,0}} \\
\hat{\alpha}(\hat{c}_{ca}) &= \frac{\alpha(c_{ca})}{\alpha(c_{ca,0})} = \frac{1+\hat{K}_{\alpha}^{n_\alpha}}{r_\alpha + \hat{K}_{\alpha}^{n_\alpha}} \frac{r_\alpha \hat{c}_{ca}^{n_\alpha} + \hat{K}_{\alpha}^{n_\alpha}}{\hat{c}_{ca}^{n_\alpha} + \hat{K}_{\alpha}^{n_\alpha}} \\
\hat{p}_{ch}(\hat{c}_{cg}) &= \frac{I_{ch,ca}(c_{cg})}{I_{ch,ca}(c_{cg,0})} = \frac{I_{ch}(c_{cg})}{I_{ch}(c_{cg,0})} = \frac{1+\hat{K}_{ch}^{n_{ch}}}{\hat{c}_{cg}^{n_{ch}} + \hat{K}_{ch}^{n_{ch}}} \hat{c}_{cg}^{n_{ch}} \\
\hat{p}_{ex}(\hat{c}_{ca}) &= \frac{I_{ex}(c_{ca})}{I_{ex}(c_{ca,0})} = \frac{1+\hat{K}_{ex}}{\hat{c}_{ca}+\hat{K}_{ex}} \hat{c}_{ca} .
\end{aligned}
\tag{6}
$$

The conditions in darkness with $\phi = 0$ are $\tilde{R}^* = \tilde{T}^* = \tilde{P}^* = 0$ and $\hat{c}_{cg} = \hat{c}_{ca} = \hat{\alpha} = \hat{p}_{ch} = \hat{p}_{ex} = 1$.

The current in Eq. 4 normalised by the dark current $I_0 = I_{ch}(c_{cg,0}) + I_{ex}(c_{ca,0}) = \frac{f_{ch,ca}+2}{2} I_{ch}(c_{cg,0}) = \frac{f_{ch,ca}+2}{f_{ch,ca}} I_{ex}(c_{ca,0})$ is

$$
\begin{aligned}
\hat{I} &= \frac{I}{I_0} = \frac{I_{ch}(c_{cg,0})}{I_0}\frac{I_{ch}(c_{cg})}{I_{ch}(c_{cg,0})} + \frac{I_{ex}(c_{ca,0})}{I_0}\frac{I_{ex}(c_{ca})}{I_{ex}(c_{ca,0})} \\
&= \frac{2}{f_{ch,ca}+2}\hat{p}_{ch}(\hat{c}_{cg}) + \frac{f_{ch,ca}}{f_{ch,ca}+2}\hat{p}_{ex}(\hat{c}_{ca}) = \hat{I}_{ch} + \hat{I}_{ex} .
\end{aligned}
\tag{7}
$$

In darkness we have $\hat{I} = 1$. We further introduce the normalized current

$$
\hat{i} = 1 - \hat{I} = \frac{I_d - I}{I_d} ,
\tag{8}
$$

which is zero in darkness. $\hat{i}$ is usually used in the literature to characterize the light response. Although we refer to $\hat{i}$ as a current (as it is usually done), it is clear that $\hat{i}$ represents the current change with respect to the dark current. $\hat{I}$ and $\hat{i}$ have complementary behaviours, for example, whereas $\hat{I}$ decreases after the light is switched on, $\hat{i}$ increases.

Before starting with the analysis of Eq. 5, we add some clarifying remarks:

1) Because we study the light response in darkness, we define the buffering constants B_{ca,b_i} using the dark Ca^{2+} concentration. With a constant background light, we would define the B_{ca,b_i} using the Ca^{2+} concentration corresponding to this background light. With high affinity buffers, this will adapt the value of the buffering capacity B_{ca} to the lower Ca^{2+} range in presence of a light background.

2) Per definition, $\frac{1+\hat{K}_{b_i})^2}{(\hat{c}_{ca}+\hat{K}_{b_i})^2}$ is one in darkness where $\hat{c}_{ca} = 1$. As we will show below, in first order it can be approximated by one for the whole dim-light response. Hence, for dim light we have $\frac{d}{dt}\hat{c}_{ca} \approx \mu_{ca}(\hat{p}_{ch} - \hat{p}_{ex})$.

3) Eq. 3 and Eq. 5 are mathematically equivalent, however, Eq. 5 depends on fewer parameters, which simplifies analysis and comprehension. Eq. 5 depends only on parameters that are important for the response dynamics. For example, Eq. 5 reveals that the activation rates k_{act}, k_{tr} and β_{sub} affect the light response only as the product $k_{act}k_{tr}\beta_{sub}$. Moreover, Eq. 5 shows that the Ca^{2+} dynamics is determined by the effective rate μ_{ca}.

4) Eq. 5 is derived assuming that the normalisation values $c_{ca,0}$ and $c_{cg,0}$ are the correct steady state concentrations in darkness ($\tilde{P}^* = 0$). Eq. 5 can be used to study the response dynamics as a function of the light intensity. In contrast, if one wants to study how the steady state is altered when parameter values are changed, Eq. 5 has to be adapted. For example, if the cyclase sensitivity is altered from $\hat{K}_\alpha$ to a new value $\hat{k}_\alpha$, the synthesis rate $\alpha(c_{ca,0})$ changes from $\alpha(c_{ca,0}) = \beta_d c_{cg,0}$ to $\alpha(c_{ca,0}) = \zeta\beta_d c_{cg,0}$, where $\zeta = \frac{r_\alpha+\hat{k}_\alpha^{n\alpha}}{1+\hat{k}_\alpha^{n\alpha}}\frac{1+\hat{K}_\alpha^{n\alpha}}{r_\alpha+\hat{K}_\alpha^{n\alpha}}$. The correct equation for $\hat{c}_{cg}$ is $\frac{d}{dt}\hat{c}_{cg} = \beta_d\zeta\hat{\alpha}(\hat{c}_{ca}) - (\beta_d + \tilde{P}^*)\hat{c}_{cg}$, with $\hat{\alpha}(\hat{c}_{ca}) = \frac{1+\hat{k}_\alpha^{n\alpha}}{r_\alpha+\hat{k}_\alpha^{n\alpha}}\frac{r_\alpha\hat{c}_{ca}^{n\alpha}+\hat{k}_\alpha^{n\alpha}}{\hat{c}_{ca}^{n\alpha}+\hat{k}_\alpha^{n\alpha}}$. It follows that $\hat{c}_{cg} = \hat{c}_{ca} = 1$ are no longer steady state solutions in darkness. The new steady values $\hat{c}_{ca}$ and $\hat{c}_{cg} = \zeta\hat{\alpha}(\hat{c}_{ca})$ are obtained by solving the equation $\hat{p}_{ch}(\zeta\hat{\alpha}(\hat{c}_{ca})) - \hat{p}_{ex}(\hat{c}_{ca}) = 0$. In a subsequent step, one can use the new steady state values to renormalise parameters, in which case one again obtains Eqs. 5,6, but with altered normalized parameters (see the analysis with modified extracellular Ca^{2+} below).

2.2 Linear response analysis for dim-light stimulations

PDE activation in Eq. 5 is linear and can be solved analytically,

$$\tilde{P}^*(t) = \int_0^t \phi(s)\kappa\xi G_p(t-s)ds, \qquad (9)$$

with the Green's function

$$G_p(t) = \frac{\mu_{rh}\mu_{tr}\mu_{pde}}{(\mu_{rh} - \mu_{tr})(\mu_{rh} - \mu_{pde})}e^{-\mu_{rh}t} + (\mu_{rh} \leftrightarrow \mu_{tr}) + (\mu_{rh} \leftrightarrow \mu_{pde}). \qquad (10)$$

The double-headed arrows in Eq. 10 signify that the second and third terms in the equation are identical to the first term with the exchange μ_{tr} and μ_{rh} in the second term, and μ_{pde} and μ_{rh} in the third term. The equations for $\hat{c}_{cg}$ and $\hat{c}_{ca}$ (Eq. 5) cannot be solved analytically for all conditions of light stimulation $\phi(t)$. However, analytic results can be derived for dim-light intensities by linearizing Eq. 5. For the analysis we introduce $y(t) = -\ln\hat{c}_{cg}(t)$ and $z(t) = -\ln\hat{c}_{ca}(t)$, which are zero in darkness. For dim-light responses with $y \ll 1$, $z \ll 1$, $\hat{p}_{ch} \approx 1 - \frac{\hat{K}_{ch}^{n_{ch}}}{1+\hat{K}_{ch}^{n_{ch}}}n_{ch}y$, $\hat{p}_{ex} \approx 1 - \frac{\hat{K}_{ex}}{1+\hat{K}_{ex}}z$, we

obtain from Eq. 5 the first-order equations

$$\frac{d}{dt}y = \tilde{P}^* - \beta_d(y + \hat{\alpha}_0' z)$$
$$\frac{d}{dt}z = \beta_d r \left(\tilde{n}_{ch} y - z\right),$$

(11)

where

$$\hat{\alpha}_0' = \left.\frac{d}{dz}\hat{\alpha}(z)\right|_{z=0} = -\left.\frac{d}{d\hat{c}_{ca}}\hat{\alpha}(\hat{c}_{ca})\right|_{\hat{c}_{ca}=1} = \frac{n_\alpha \hat{K}_\alpha^{n_\alpha}(1-r_\alpha)}{(1+\hat{K}_\alpha^{n_\alpha})(\hat{K}_\alpha^{n_\alpha}+r_\alpha)}$$

$$\tilde{n}_{ch} = \frac{1+\hat{K}_{ex}}{\hat{K}_{ex}}\frac{\hat{K}_{ch}^{n_{ch}}}{1+\hat{K}_{ch}^{n_{ch}}}n_{ch}$$

(12)

$$r = \frac{\mu_{ca}}{\beta_d}\frac{\hat{K}_{ex}}{1+\hat{K}_{ex}}.$$

For GCAPs$^{-/-}$ mutants the cyclase is not Ca^{2+} dependent and we have $\hat{\alpha}_0' = 0$. The two independent solutions of Eq. 11 with $\tilde{P}^* = \int_0^t \phi(s)\kappa\xi G_p(t-s)ds$ are

$$y(t) = \sum_{i=1}^2 \zeta_{y,i}\int_0^t \phi(s)\kappa\xi G_i(t-s)ds, \quad z(t) = \sum_{i=1}^2 \zeta_{z,i}\int_0^t \phi(s)\kappa\xi G_i(t-s)ds,$$

(13)

where $\zeta_{y,1} = \frac{r-\lambda_1}{\lambda_2-\lambda_1}$, $\zeta_{y,2} = \frac{r-\lambda_2}{\lambda_1-\lambda_2}$, $\zeta_{z,1} = \frac{\tilde{n}_{ch}r}{\lambda_2-\lambda_1}$ and $\zeta_{z,2} = \frac{\tilde{n}_{ch}r}{\lambda_1-\lambda_2}$. The parameters $\lambda_1 = \frac{1+r}{2} - \frac{\sqrt{(r-1)^2-4\tilde{n}_{ch}\hat{\alpha}_0'r}}{2}$ and $\lambda_2 = \frac{1+r}{2} + \frac{\sqrt{(r-1)^2-4\tilde{n}_{ch}\hat{\alpha}_0'r}}{2}$ are the eigenvalues of the matrix $\begin{pmatrix} 1 & \hat{\alpha}_0' \\ -\tilde{n}_{ch}r & r \end{pmatrix}$. The two independent Green's functions are $(i = 1, 2)$

$$G_i(t) = -\frac{\mu_{rh}\mu_{tr}\mu_{pde}e^{-\mu_{rh}t}}{(\mu_{rh}-\mu_{tr})(\mu_{rh}-\mu_{pde})(\mu_{rh}-\beta_d\lambda_i)} + (\mu_{rh}\leftrightarrow\mu_{tr}) + (\mu_{rh}\leftrightarrow\mu_{pde}) + (\mu_{rh}\leftrightarrow\beta_d\lambda_i)$$
$$= G_{rh}(t) + G_{tr}(t) + G_{pde}(t) + G_{\beta_i}(t),$$

(14)

where the double-headed arrows have the same significance as previously. For a step of light at $t = 0$ with duration Δt and constant intensity ϕ we get $y(t) = R_0^*\xi g_y(t)$ and $z(t) = R_0^*\xi g_z(t)$, where $R_0^* = \kappa\phi\Delta t$ are the number of isomerisations and

$$g_y(t) = \sum_{i=1}^2 \zeta_{y,i}\frac{1}{\Delta t}\int_0^{\min(t,\Delta t)} G_i(t-s)ds, \quad g_z(t) = \sum_{i=1}^2 \zeta_{z,i}\frac{1}{\Delta t}\int_0^{\min(t,\Delta t)} G_i(t-s)ds.$$

(15)

From Eqs. 7-8 we obtain the current $\hat{i}(t) = 1 - \frac{2}{f_{ch,ca}+2}\hat{p}_{ch} - \frac{f_{ch,ca}}{f_{ch,ca}+2}\hat{p}_{ex} \approx \frac{2}{f_{ch,ca}+2}\frac{\hat{K}_{ch}^{n_{ch}}}{1+\hat{K}_{ch}^{n_{ch}}}n_{ch}y(t) + \frac{f_{ch,ca}}{f_{ch,ca}+2}\frac{\hat{K}_{ex}}{1+\hat{K}_{ex}}z(t) = R_0^*\hat{i}_{spr}(t)$, where

$$\hat{i}_{spr}(t) = \xi n_{ch}\frac{\hat{K}_{ch}^{n_{ch}}}{1+\hat{K}_{ch}^{n_{ch}}}\frac{2}{f_{ch,ca}+2}\left(g_y(t) + \frac{f_{ch,ca}}{2\tilde{n}_{ch}}g_z(t)\right).$$

(16)

For short flashes with duration $\Delta t \to 0$, $\hat{i}_{spr}$ corresponds to the classical single-photon response (SPR). For light steps with duration Δt, $\hat{i}_{spr}$ is a unitary response for steps with duration Δt.

We use Eq. 14 to decompose the current into different parts that reflect the contributions from the various biophysical processes,

$$\hat{i}_{spr} = \hat{i}_{spr,rh} + \hat{i}_{spr,tr} + \hat{i}_{spr,pde} + \hat{i}_{spr,\beta_1} + \hat{i}_{spr,\beta_2} = \hat{i}_{spr,rh} + \hat{i}_{spr,tr} + \hat{i}_{spr,pde} + \hat{i}_{spr,\beta} \,. \tag{17}$$

For the SPR with $\Delta t \to 0$ we have $\frac{1}{\Delta t} \int_0^{\min(t,\Delta t)} G_i(t-s) \approx G_i(t)$, such that $\hat{i}_{spr,rh} \sim e^{-\mu_{rh}t}$, $\hat{i}_{spr,tr} \sim e^{-\mu_{tr}t}$, $\hat{i}_{spr,pde} \sim e^{-\mu_{pde}t}$, $\hat{i}_{spr,\beta_1} \sim e^{-\beta_d\lambda_1 t}$, and $\hat{i}_{spr,\beta_2} \sim e^{-\beta_d\lambda_2 t}$.

In the limit $\mu_{ca} \to \infty$ ($r \to \infty$) we have $\lambda_1 \to 1 + \tilde{n}_{ch}\hat{\alpha}'_0$ and $\lambda_2 \to \infty$, and we obtain $\hat{i}_{spr,\beta} \sim e^{-\beta_d\lambda_1 t}$, in agreement with [35]. With fast Ca^{2+} kinetics we further have $\hat{p}_{ch} \approx \hat{p}_{ex}$ and $\hat{I} \approx \hat{p}_{ex} \approx \hat{c}_{ca}$ (the latter is valid for $\hat{K}_{ex} \gg 1$), showing that in this limit the Ca^{2+} concentration changes in proportion to the current. In the opposite limit $\mu_{ca} \to 0$ ($r \to 0$), we have $\lambda_1 \to 1$, $\lambda_2 \to 0$, $\zeta_{y,2} \to 0$, $\zeta_{z,2} \to 0$, such that $\hat{i}_{spr,\beta} \sim e^{-\beta_d t}$. The same behaviour is obtained for the GCAPs$^{-/-}$ case with $\hat{\alpha}'_0 = 0$ ($\lambda_1 = 1$).

2.2.1   Emergence of damped oscillations

For $(r-1)^2 - 4\tilde{n}_{ch}\hat{\alpha}'_0 r < 0$, the eigenvalues λ_i are complex conjugate, and $\hat{i}_{spr,\beta} = \hat{i}_{spr,\beta_1} + \hat{i}_{spr,\beta_2}$ describes a damped oscillation. Such oscillations arise for $r_1 < r < r_2$, with the bifurcation points $r_1 = 1 + 2\tilde{n}_{ch}\hat{\alpha}'_0 \left(1 - \sqrt{1 + \frac{1}{\tilde{n}_{ch}\hat{\alpha}'_0}}\right)$ and $r_2 = 1 + 2\tilde{n}_{ch}\hat{\alpha}'_0 \left(1 + \sqrt{1 + \frac{1}{\tilde{n}_{ch}\hat{\alpha}'_0}}\right)$. By writing $\lambda_1 = \lambda_{re} - i\lambda_{im}$ and $\lambda_2 = \lambda_{re} + i\lambda_{im}$, with $\lambda_{re} = \frac{1+r}{2}$ and $\lambda_{im} = \frac{\sqrt{-(r-r_1)(r-r_2)}}{2}$, we obtain for a short flash

$$\hat{i}_{spr,\beta} = \xi n_{ch} \frac{\hat{K}_{ch}^{n_{ch}}}{1 + \hat{K}_{ch}^{n_{ch}}} \frac{2}{f_{ch,ca}+2} \left(a_y \cos(\omega t + \varphi_y) + \frac{f_{ch,ca}}{2\tilde{n}_{ch}} a_z \cos(\omega t + \varphi_z)\right) e^{-\mu_{damp}t} \,, \tag{18}$$

with oscillation frequency $\omega = \beta_d \lambda_{im} = \beta_d \frac{\sqrt{(r-r_1)(r_2-r)}}{2}$ and damping rate $\mu_{damp} = \beta_d \lambda_{re} = \beta_d \frac{1+r}{2} = \frac{\beta_d + \mu_{ca}\frac{\hat{K}_{ex}}{1+\hat{K}_{ex}}}{2}$. The oscillation amplitudes a_y and a_z, and the phases φ_y and φ_z can be computed with Eq. 14.

2.2.2   Steady state with a dim background light

With constant light intensity ϕ we have $\hat{p}_{ch} = \hat{p}_{ex}$ and $\hat{I} = \hat{p}_{ch} = \hat{p}_{ex}$. The steady state solutions of Eq. 11 are $z = \tilde{n}_{ch}y$ and $y = \frac{\phi\kappa\xi}{\beta_d(1+\tilde{n}_{ch}\hat{\alpha}'_0)}$. For the current we get $\hat{i} = 1 - \hat{I} = 1 - \hat{p}_{ch} \approx \frac{\hat{K}_{ch}^{n_{ch}}}{1+\hat{K}_{ch}^{n_{ch}}} n_{ch}y = \frac{\hat{K}_{ch}^{n_{ch}}}{1+\hat{K}_{ch}^{n_{ch}}} \frac{\kappa\xi n_{ch}}{\beta_d(1+\tilde{n}_{ch}\hat{\alpha}'_0)}\phi$.

2.3   Changing the extracellular Ca^{2+} concentration

We now investigate how the photoresponse is modified when the extracellular Ca^{2+} concentration is altered by a factor of $r_{ca,ex}$ compared to the previous reference concentration ($r_{ca,ex} = 1$). We assume that the CNG current carried by Ca^{2+} changes in proportion to the extracellular concentration, $\hat{I}_{ch,ca} = r_{ca,ex}f_{ch,ca}\frac{2}{f_{ch,ca}+2}\hat{p}_{ch}$, whereas the current not carried by Ca^{2+} remains unaffected, $\hat{I}_{ch,\overline{ca}} = (1-f_{ch,ca})\frac{2}{f_{ch,ca}+2}\hat{p}_{ch}$. Thus, the CNG current is $\hat{I}_{ch} = \hat{I}_{ch,ca} + \hat{I}_{ch,\overline{ca}} = \frac{\hat{I}_{ch,ca}}{f'_{ch,ca}}$, where

$$f'_{ch,ca} = f_{ch,ca}\frac{r_{ca,ex}}{1 + (r_{ca,ex}-1)f_{ch,ca}} \tag{19}$$

is the new fraction of the CNG current carried by Ca^{2+} ($f_{ch,ca}$ is reference value from Table 1 for $r_{ca,ex} = 1$). The overall current is

$$\hat{I} = \hat{I}_{ch} + \hat{I}_{ex} = \frac{r_{ca,ex}f_{ch,ca}}{f'_{ch,ca}}\frac{2}{f_{ch,ca}+2}\hat{p}_{ch}(\hat{c}_{cg}) + \frac{f_{ch,ca}}{f_{ch,ca}+2}\hat{p}_{ex}(\hat{c}_{ca}). \tag{20}$$

With $\hat{I}_{ch,ca} = r_{ca,ex}f_{ch,ca}\frac{2}{f_{ch,ca}+2}\hat{p}_{ch}$, the equation for $\hat{c}_{ca}$ now reads

$$\frac{d}{dt}\hat{c}_{ca} = \frac{1+B_{ca}}{1+\sum_{i=1}^{N_b}B_{ca,b_i}\frac{(1+\hat{K}_{b_i})^2}{(\hat{c}_{ca}+\hat{K}_{b_i})^2}}\mu_{ca}\left(r_{ca,ex}\hat{p}_{ch}(\hat{c}_{cg}) - \hat{p}_{ex}(\hat{c}_{ca})\right). \tag{21}$$

Thus, for $r_{ca,ex} \neq 1$ we have that $\hat{c}_{ca} = \hat{c}_{cg} = 1$ are no longer steady state solutions in darkness. The new steady state values $\hat{c}_{ca,d}$ and $\hat{c}_{cg,d} = \hat{\alpha}(\hat{c}_{ca,d})$ are obtained by solving the equation $r_{ca,ex}\hat{p}_{ch}(\hat{\alpha}(\hat{c}_{ca,d})) - \hat{p}_{ex}(\hat{c}_{ca,d}) = 0$. With $\hat{p}_{ex} = r_{ca,ex}\hat{p}_{ch}$ we obtain from Eq. 20 for the dark current

$$\hat{I}_d = \left(1 - \frac{3f_{ch,ca}(1-r_{ca,ex})}{f_{ch,ca}+2}\right)\frac{1+\hat{K}_{ch}^{n_{ch}}}{\hat{c}_{cg}^{n_{ch}} + \hat{K}_{ch}^{n_{ch}}}\hat{c}_{cg}^{n_{ch}}. \tag{22}$$

Finally, with $f'_{ch,ca}$, and with parameters that are normalized with the new steady state values $\hat{c}_{ca,d}c_{ca,0}$, $\hat{c}_{cg,d}c_{cg,0}$ and $\hat{I}_d I_0$, we can use Eq. 5 and Eq. 6 with modified parameters to study the response with modified extracellular Ca^{2+}. .

3 Results

Eq. 5 reveals that the Ca^{2+} kinetics is controlled by the effective rate $\mu_{ca} = \frac{1}{(1+B_{ca})F_A V_{os}}\frac{I_{ex}(c_{ca,d})}{c_{ca,d}}$ (Eq. 6). The value of μ_{ca} depends on the effective buffering constant $B_{ca} = \sum_{i=1}^{N_b} B_{ca,b_i}$, which adds the contributions from the various buffer species. With $B_{ca} = 0$ and parameters from Table 1 we compute $\mu_{ca} \sim 1.6 \times 10^3 s^{-1}$ for a rod, and $\mu_{ca} \sim 9.4 \times 10^3 s^{-1}$ for a cone. With fast Ca^{2+} kinetics (large μ_{ca}) we have $\hat{p}_{ch} \approx \hat{p}_{ex}$, and the time-dependent current can be approximated by the steady state expression $\hat{I} \approx \hat{p}_{ch} \approx \hat{p}_{ex}$. Moreover, for $\hat{K}_{ex} \gg 1$ we have $\hat{p}_{ex} \approx \hat{c}_{ca}$ and $\hat{c}_{ca} \approx \hat{I}$. Thus, for large μ_{ca} and $\hat{K}_{ex} \gg 1$ we find that the Ca^{2+} concentration changes in proportion to the current. In this limit we recover our results from [34, 35].

We now generalize our previous results by studying the photoresponse as a function of μ_{ca}. A straightforward experimental method to slow down the Ca^{2+} dynamics is to add exogenous buffers. This leads to a larger buffering capacity B_{ca} and a reduced μ_{ca}, but otherwise does not modify Eqs. 5,6. In contrast, modifying exchanger properties affects μ_{ca} and steady state values. To study such a case, one would have to first adapt Eqs. 5,6. Nevertheless, in the following we use the value of μ_{ca} to characterize the difference between responses (and not B_{ca}), because it is the value of μ_{ca} with respect to other rate constants of the model that is relevant.

3.1 Validity range of the analytic results

We check the validity range of our asymptotic analysis by comparing simulations and analytic results for $\hat{i}$. For the simulations, we use Eq. 5 with one low and high affinity buffer each, as specified in Table 1 (recoverin and GCAPs). The buffering parameters in Table 1 are obtained as follows: Recoverin is the most abundant calcium buffer in the outer segment [6, 55], with a dissociation constant $K_{ca,rec} \sim 3\mu M$ [54]. To obtain a realistic buffering constant around $B_{ca} \sim 40 - 50$ [47], we

estimate that the recoverin concentration has to be around $c_{rec} \sim 150\mu M$. Such values are consistent with estimations from [26, 56]. For GCAPs buffering we use $c_{gcaps} \sim 3\mu M$ with a dissociation constant $K_{ca,gcaps} \sim 0.14\mu M$ [55]. For the buffering, GCAPs contributes to B_{ca} only a small value around $3 \times 0.14/(0.3 + 0.14)^2 \sim 2$. Note that we consider the effect of binding between Ca^{2+} and recoverin for the buffering, but we neglect the effect of Ca^{2+} binding to recoverin for photopigment deactivation. The latter further depends on the interaction between rhodopsin kinase and recoverin, which we assume to occur on a much slower time scale.

To check the validity range of our asymptotic analysis, we compare simulations and analytic results for $\hat{i}$ for short flashes and longer step responses with fast and slow Ca^{2+} kinetics, characterized by μ_{ca}, for rods (Fig. 1) and cones (Fig. 2). Simulations are computed with Eq. 5, analytic results are $\hat{i} = R_0^* \hat{i}_{spr}$, where $R_0^* = \phi\kappa\Delta t$ are the number isomerisations produced by ϕ during the stimulation time Δt, and $\hat{i}_{spr}$ is from Eq. 16. The values for μ_{ca} displayed in Fig. 1A and Fig. 2B are computed with Eq. 6 using parameters from Table 1. For the simulations with tenfold reduced μ_{ca}, we simply increase both buffer concentrations by a factor of 10.

For dim light, simulations and analytic results for rods and cones faithfully agree for flash responses with fast and slow Ca^{2+} dynamics (Fig. 1A-B and Fig. 2A-B, black vs red curves), as well as step responses (Fig. 1C-D and Fig. 2C-D, black vs red curves). As the light intensity increases, the analytic result overestimates the current response because the linear approximation underestimates the non-linear increase in the negative Ca^{2+} feedback to the cyclase. For large μ_{ca} ($\mu_{ca} = 37s^{-1}$ for rod, $\mu_{ca} = 210s^{-1}$ for cone) we observe monophasic responses (Fig. 1A,C and Fig. 2A,C). With 10-fold increased buffering ($\mu_{ca} = 3.7s^{-1}$ for rod, $\mu_{ca} = 21s^{-1}$ for cone) we observe damped oscillations (Fig. 1B,D and Fig. 2B,D), as predicted by Eq. 18. In summary, this shows that our analytic formulas can be applied to study the dim-light response.

3.2 Single photon response (SPR) and unitary step response

Because dim-light responses are proportional the number of isomerisations $R_0^* = \phi\kappa\Delta t$, we focus on the unitary response $\hat{i}_{spr}$ with $R_0^* = 1$ (Eq. 16). For short flashes with $\Delta t \to 0$, $\hat{i}_{spr}$ corresponds to the classical single-photon response (SPR). For steps with longer duration Δt, the unitary step response $\hat{i}_{spr}$ is a response function (a single isomerisation can never produce a step response).

We find that time to peak and amplitude of a SPR decrease as μ_{ca} increases, because a faster Ca^{2+} dynamics leads to quicker cyclase activation and more negative feedback (Fig. 3A,B). Thus, a slower Ca^{2+} dynamics implies a larger rod sensitivity (larger amplitude), in agreement with experiments with exogenous buffering [14]. In GCAPs$^{-/-}$ photoreceptors where the Ca^{2+} feedback to the cyclase is genetically removed, the Ca^{2+} kinetics affects the light response only little via the exchanger current (Fig. 3A-B, dashed lines). This shows that the Ca^{2+} dynamics affects the dim-light response mainly because of the cyclase feedback, in agreement with experiments [17].

Next we characterize the different phases of a flash and step response. For flash responses, we define the initial phase up to the peak time, and the recovery phase afterwards (Fig. 3A-B). For step responses where Δt is sufficiently long such that an intermediate steady state is reached, we define the initial phase up to the time when the intermediate plateau value is reached; afterwards we define the plateau phase up to the time when the light is switched off, and finally we have the recovery phase (Fig. 3C-D). Slowing down the Ca^{2+} kinetics increases both amplitude and time to peak of a SPR, and damped oscillations start to appear during the recovery phase (Fig. 3A-B) (see the analysis in section 2.2.1). For a step response, only initial and recovery phases depend on μ_{ca}, whereas the plateau phase is determined by steady-state properties that do not depend on μ_{ca} (Fig. 3C-D, solid lines). We compute that the GCAPs$^{-/-}$ plateau current is by a factor of $1 + \tilde{n}_{ch}\hat{\alpha}_0'$ larger compared

to the WT value (see the analysis after Eq. 18). With Table 1, we find $\tilde{n}_{ch} \approx 2.92$, $\hat{\alpha}'_0 \approx 1.37$ and $1 + \tilde{n}_{ch}\hat{\alpha}'_0 \approx 5$. Thus, whereas the plateau currents between WT and GCAPs$^{-/-}$ step responses differ by a factor of around 5 (Fig. 3C-D), the WT and GCAPs$^{-/-}$ SPR amplitudes depend on μ_{ca} and differ maximally by a factor of around 2-3 with fast Ca^{2+} kinetics (Fig. 3A-B).

3.3 Waveform of flash and step responses

Changing the Ca^{2+} kinetics affects amplitude and shape of flash and step responses (Fig. 3). To compare how the response shape is affected, we use waveforms where the response amplitude is normalized to one. For short flashes (see Fig. 3A-B), we define the current waveform by normalizing $\hat{i}(t) = 1 - \hat{I}(t)$ with the peak amplitude. For longer step responses (see Fig. 3C-D), we define the waveform by normalizing $\hat{i}(t)$ with the intermediate plateau value. To compare current and Ca^{2+} changes, we define the Ca^{2+} waveform using the change in the Ca^{2+} concentration $1 - \hat{c}_{ca}(t)$. For dim light we have $1 - \hat{c}_{ca}(t) \approx z(t)$.

The current waveform is monophasic for large μ_{ca} (Fig. 4A-B, magenta curves), and in this limit the Ca^{2+} concentration changes in proportion to the current (Fig. 4C-D, green curves). As μ_{ca} decreases, damped oscillations emerge (Fig. 4A-B) because the Ca^{2+} dynamics becomes more and more delayed with respect to the current (Fig. 4C-D, red and black curves). In limit $\mu_{ca} \to 0$ the current response becomes monophasic because Ca^{2+} concentration and cyclase activity remain constant (nor shown, but see also the GCAPs$^{-/-}$ responses in Fig. 3).

Whereas the flash shape differs between initial and recovery phase (Fig. 4A), there is a symmetry between these phases for step responses (Fig. 4B). Indeed, when an intermediate steady state is reached, we find from Eq. 11 that initial and recovery phase are related by $\hat{i}_{step}(\Delta t + t) = \hat{i}_{ss} - \hat{i}_{step}(t)$, where $\hat{i}_{ss}$ is the intermediate steady state current.

3.4 Waveform decomposition

Next we use the analytic result in Eq. 17 to show how the various biophysical processes contribute to the response. Such information cannot be obtained from simulations. We find that the recovery in a rod with fast Ca^{2+} dynamics is limited by PDE decay, $\hat{i}_{spr,pde} \sim e^{-\mu_{pde}t}$(Fig. 5A)). For a GCAPs$^{-/-}$ cone we have that the recovery is limited by the basal turnover rate β_d, $\hat{i}_{spr,\beta} \sim e^{-\beta_d t}$ (Fig. 5B. For these two cases, parameters can be extracted by fitting the response recovery with a single exponential. In general, however, the recovery of flash responses is not determined by a single exponential. For example, with slow Ca^{2+} dynamics the recovery phase contains a damped oscillations (Fig. 5C-D), in which case fitting the response decay with a single exponential does not yield meaningful parameter values.

3.5 Damped oscillations

The analysis in section 2.2.1 shows that the response contains a damped oscillation if the ratio $r = \frac{\mu_{ca}}{\beta_d} \frac{\hat{K}_{ex}}{1 + \hat{K}_{ex}} \approx \frac{\mu_{ca}}{\beta_d}$ is within the range $r_1 < r < r_2$, where $r_1 = 1 + 2\tilde{n}_{ch}\hat{\alpha}'_0 \left(1 - \sqrt{1 + \frac{1}{\tilde{n}_{ch}\hat{\alpha}'_0}}\right)$ and $r_2 = 1 + 2\tilde{n}_{ch}\hat{\alpha}'_0 \left(1 + \sqrt{1 + \frac{1}{\tilde{n}_{ch}\hat{\alpha}'_0}}\right)$ depend on the CNG channel cooperativity n_{ch} and the sensitivity of the cyclase to Ca^{2+} α'_0 (see section 2.2.1). For example, with Table 1 we compute $\tilde{n}_{ch} \approx 2.9$, $\hat{\alpha}'_0 \approx 1.37$, $r_1 \approx 0.05$ and $r_2 \approx 18$. The rage for μ_{ca} where oscillations occur, determined by $\beta_d \frac{1 + \hat{K}_{ex}}{\hat{K}_{ex}} r_1 < \mu_{ca} < \beta_d \frac{1 + \hat{K}_{ex}}{\hat{K}_{ex}} r_2$, increases as a function of the channel cooperativity and cyclase feedback $\tilde{n}_{ch}\hat{\alpha}'_0$ (Fig. 6A; cone (black curve) and rod (red curve)). This range is wider for a cone

because of the larger β_d (Fig. 6A). No oscillations occur for Gcaps$^{-/-}$ mutants with $\tilde{n}_{ch}\hat{\alpha}'_0 = 0$. The oscillation frequency depends on μ_{ca}, $\omega = \beta_d \frac{\sqrt{(r-r_1)(r_2-r)}}{2}$ (Eq. 18). As function of μ_{ca}, ω increases from zero towards the maximal frequency $\omega_{max} = \frac{r_2-r_1}{4} \approx \beta_d \frac{r_2}{4}$, which is attained for $r = \frac{r_1+r_2}{2} \approx \frac{r_2}{2}$ and $\mu_{ca} \approx \beta_d r \approx \beta_d \frac{r_2}{2} \approx 2\omega_{max}$. Afterwards, ω decreases again as μ_{ca} further increases (Fig. 6B).

Although oscillations occur over a wide range of μ_{ca} values (Fig. 6A), they affect the recovery phase only if the damping rate $\mu_{damp} = \beta_d \frac{1+r}{2} \approx \frac{\beta_d+\mu_{ca}}{2}$ is not too large. Indeed, for large μ_{ca} oscillations are damped before they reach the recovery phase (Fig. 5A, magenta curve). As μ_{ca} decreases, oscillations start to affect the recovery phase (Fig. 5C-D). It is difficult to give a precise value for μ_{ca} that indicates when oscillations start to become visible during the recovery phase, which depends on damping but also the initial amplitude of the oscillation. We note, however, that for large $r \approx \frac{\mu_{ca}}{\beta_d}$ where the Ca^{2+} dynamics is determined by the current, the response changes only slowly as a function of r (see Fig. 3A-B). More profound changes start to occur for $r \lesssim \frac{r_1+r_2}{2} = 1 + 2\tilde{n}_{ch}\hat{\alpha}'_0$, where $\frac{r_1+r_2}{2}$ corresponds to the center of the oscillation ranges Fig. 6A. From this we obtain that the response becomes significantly altered for $\mu_{ca} \lesssim \beta_d r^* \approx 9\beta_d$, which seems compatible with Fig. 3A-B.

3.6 Effect of changing the extracellular Ca^{2+} concentration

Finally, we explored how changing the extracellular Ca^{2+} concentration affects the light response in a cone (similar conclusions apply for a rod, not shown). We consider that the extracellular concentration is altered by a factor of $r_{ca,ex}$ compared to the previous reference value, which alters the fraction of the CNG current that is carried by Ca^{2+} by a factor of $\hat{f}_{ch,ca} = \frac{r_{ca,ex}}{1+(r_{ca,ex}-1)f_{ch,ca}}$ (see Eq. 19), where $f_{ch,ca} = 0.3$ is the reference value for $r_{ca,ex} = 1$. As a consequence of the modified Ca^{2+} influx, the dark steady-state values $\hat{c}_{ca,d}$, $\hat{c}_{cg,d}$ and $\hat{I}_d$ also change (Fig. 7A, black, red and blue curves). For example, when the extracellular Ca^{2+} concentration is lowered tenfold ($r_{ca,ex} = 0.1$), the fraction of the CNG current that is carried by Ca^{2+} is reduced by a factor of around 7 ($\hat{f}_{ca,ca} \approx 0.14$). The dark Ca^{2+} concentration in the OS is reduced by a factor of around 2 ($\hat{c}_{ca,d} \approx 0.55$), which activates the cyclase and results in an around 2.1-fold higher cGMP concentration ($\hat{c}_{cg,d} \approx 2.1$), and an around 3.8-fold larger dark current ($\hat{I}_d \approx 3.8$). In contrast, the value of μ_{ca} changes only little because $\frac{I_{ex}}{c_{ca}}$ is almost constant for $K_{ex} \gg c_{ca}$, and because recoverin has a low Ca^{2+} affinity (Table 1), such that B_{ca} is only little affected by the reduction in Ca^{2+}.

To study the dynamics of $\hat{i}_{spr}$ with $r_{ca,ex} = 0.1$, we use Eq. 16 with parameters that are normalized with the new steady state values, and with the new value for $f_{ch,ca}$. We find that a tenfold reduction of extracellular Ca^{2+} slightly increases the normalized amplitude and the duration of the SPR (Fig. 7B; solid curves are for $r_{ca,ex} = 0.1$, dashed curves for $r_{ca,ex} = 1$). Since μ_{ca} is not much changed, this effect is due to the smaller cyclase feedback $\hat{\alpha}'_0$, which is reduced from the reference value $\hat{\alpha}'_0 \approx 1.38$ ($r_{ca,ex} = 1$) to $\hat{\alpha}'_0 \approx 1.07$ ($\hat{K}_\alpha = \frac{K_\alpha}{\hat{c}_{ca,d}c_{ca,0}}$ is larger for $r_{ca,ex} = 0.1$). Although the normalized responses are not much different, because of the 3.8-fold larger dark current ($I_d = 15pA$ for $r_{ca,ex} = 1$ (Table 1); $I_d = 3.8 \times 15pA$ for $r_{ca,ex} = 0.1$) the amplitude of the SPR current $i_{spr} = \hat{i}_{spr}I_d$ is much increased with reduced extracellular Ca^{2+} (Fig. 7C, solid vs dashed curves). By comparing the current waveforms for $\mu_{ca} = 50s^{-1}$, we find the the undershoot is slightly reduced for $r_{ca,ex} = 0.1$ (Fig. 7D).

4 Discussion

The signal transduction pathway of rod and cone photoreceptors consists of a cascade of biophysical processes that transform light into a current response. Many of these steps depend on Ca^{2+} feedback, which can be manipulated by exogenous buffers, or by changing the extracellular Ca^{2+} concentration.

So far, the impact of Ca^{2+} on the response dynamics has mostly been studied using numerical simulations [36, 37, 57, 44, 58, 27]. In this work, we derived analytic results for dim-light responses in rods and cones that show how response sensitivity and dynamics change as the Ca^{2+} kinetics is altered due to fast buffering and change in the extracellular Ca^{2+} concentration. Our analytic formulas not only provide quantitative and conceptual insight, but they are also a means to easily compute photoreceptor responses based on underlying biophysical parameters without having to numerically solve a system of differential equations, which can be used as input to study downstream processes in the retina [59].

We found that the Ca^{2+} kinetics in presence of fast buffering is controlled the effective rate $\mu_{ca} = \frac{I_{ex,d}}{(1+B_{ca})F_A V_{os} c_{ca,d}}$ (Eq. 6). B_{ca} is an effective buffering constant that has contributions from the various buffer species (Eq. 6), V_{os} is the outer segment volume, $I_{ex,d}$ is the exchanger current in darkness, $c_{ca,d}$ is the dark Ca^{2+} concentration, and F_A is the Faraday constant. For large μ_{ca}, light responses are monophasic (Fig. 3, magenta curves) and the Ca^{2+} concentration changes in proportion to the current (Fig. 4C-D, green curves). As μ_{ca} decreases, the Ca^{2+} concentration becomes delayed with respect to the current (Fig. 4C-D, red and black curves), and damped oscillations emerge (Fig. 4A-B). Our analysis shows that fast buffering alone can induce oscillations, and the presence of slow buffers is not mandatory.

The phase space analysis reveals that the transition form monophasic to biphasic (oscillatory) responses depends on the ratio μ_{ca}/β_d. Oscillations occur if this ratio is below a threshold value of around 18, which depends on the strength of the cyclase feedback $\hat{\alpha}'_0$, and the channel cooperativity n_{ch}. Because β_d is much larger in a mouse cone compared to rod [34], the range for μ_{ca} where oscillations can occur is much larger in a cone (Fig. 6A). The differences in β_d might be one of the reasons why oscillations are rarely observed in amphibian compared to primate rods [37], and why they have been more frequently observed in cones [29, 30, 31]. We further computed that oscillations are damped with rate $\mu_{damp} \approx \frac{\beta_d + \mu_{ca}}{2}$, and we determined the oscillation frequency as a function of μ_{ca} (Fig. 6B). Although the range of μ_{ca} where oscillations occur is large (Fig. 6A), oscillations are visible during the recovery phase of flash responses only if the damping is not too strong, which requires that the Ca^{2+} kinetics is sufficiently slowed down (compare the magenta curves in Fig. 5A,C).

With the analytic results it is possible to decompose the dim-flash response into individual terms that reflect contributions from various biophysical processes (Eq. 17 and Fig. 5). Such a decomposition cannot be performed with simulations only. As expected, the decomposition shows that oscillations are present in the term that describes the interaction between Ca^{2+} and cGMP synthesis (Fig. 5, magenta curves). In GCAPs$^{-/-}$ photoreceptors where this interaction is absent, flash responses are monophasic, and they vary only little with μ_{ca} (Fig. 3 dashed lines), in agreement with experiments [17]. The small dependency on μ_{ca} for GCAPs$^{-/-}$ photoreceptors is a consequence of Ca^{2+}-dependent exchanger current. In WT photoreceptors with intact cyclase feedback, modifying the Ca^{2+} kinetics strongly affects amplitude and shape of the light response (Fig. 3, solid lines). The sensitivity (amplitude) of the single-photon response (SPR) increases gradually as the Ca^{2+} kinetics is slowed down (Fig. 3A-B, solid lines), which is because the negative Ca^{2+} feedback to the cyclase becomes delayed (Fig. 4C). This agrees with larger photoreceptor sensitivities observed with exogenous buffering [14]. We find a maximal sensitivity ratio around 2-3 between GCAPs$^{-/-}$ and WT photoreceptors for fast Ca^{2+} kinetics. Because the observed sensitivity ratio between GCAPs$^{-/-}$ and WT photoreceptors is around 3 [34, 17, 52], this suggests that under physiological conditions the Ca^{2+} kinetics is fast, and that the Ca^{2+} concentration changes in proportion to the current [51, 60].

For step responses with an intermediate plateau phase, oscillations are visible during the initial and recovery phase of the response (Fig. 4B). The plateau value is determined by steady-state properties and independent of the Ca^{2+} kinetics. We computed that the plateau value in a GCAPs$^{-/-}$

photoreceptor is by a factor of $1 + n_{ch}\hat{\alpha}'_0 \sim 5$ larger compared to WT (Fig. 3C-D). Since this ratio is independent of the Ca^{2+} kinetics, it could be used to estimate the strength of the cyclase feedback $\hat{\alpha}'_0$. Whereas initial and recovery phase of flash responses are different (Fig. 4A), there is a symmetry between these phases for step responses (Fig. 4B); see also Fig. 5B in [61]). Hence, the analysis of initial and recovery phase of dim step responses provides the same information, whereas complementary information can be extracted from flash response (see [35]).

We explored how reducing the extracellular Ca^{2+} concentration affects the SPR response in a cone (similar conclusions apply to rod, not shown). Modifying extracellular Ca^{2+} alters the fraction $f_{ch,ca}$ of the CNG current that is carried by Ca^{2+} (Eq. 19), and thereby changes the steady state values of Ca^{2+}, cGMP and current (Fig. 7A). For example, a tenfold reduction in extracellular Ca^{2+} reduces the dark Ca^{2+} concentration by a factor of 2, it increases the SPR amplitude by a factor of 3.8 (Fig. 7A), and it prolongs the SPR duration (Fig. 7B). Similar changes have been observed experimentally for primate cones when the extracellular Ca^{2+} concentration has been reduced (Fig. 2A in [33]). In [33] it has also occasionally been observed that a biphasic response could be transformed into a monophasic response by lowering the extracellular Ca^{2+} concentration (Fig. 2A in [33]). Although we also observe a small reduction of the undershoot (Fig. 7C), the effect seems much weaker than shown in [33]. A possible reason for this could be that, occasionally, the reduction in the extracellular Ca^{2+} concentration leads to a complete saturation of the cyclase, which abolishes the oscillation and gives monophasic responses.

In this work we did not consider slow buffers in order to keep the analysis most comprehensible. However, it is straightforward to generalize the analysis with slow buffering in future work. In first approximation, and with a single slow buffer species, Eq. 11 will be replaced by 3-dimensional system of equations. Although the phase space is now more complex, we do not expect to find solutions that are qualitatively much different from what we have observed here, which is consistent with simulations in presence of slow buffering reactions [36, 37]

We used a non-spatial (well-stirred) model for the outer segment, which allowed to derive analytic results. Non-spatial models are frequently used to study the photoresponse [34, 62, 42, 41, 27, 40, 63, 58, 64, 44, 43, 36]. Whereas spatial models are a more accurate description of reality, the downside is that no analytic results can usually be derived [65, 49, 48, 46, 66, 67]. Nevertheless, we performed simulations with our spatial model from [48] to check that our conclusions remain valid (not shown). Recently it has been found that the large outer segment of a frog rod is a spatially inhomogeneous compartment [60, 68]. It remains unclear whether this is also true for the much smaller outer segment of mouse or primate rods and cones. We leave it for future work to investigate how a possible spatial inhomogeneity might affect the photoresponse.

Although we focused on the dim-light response in darkness, the linear response analysis that we presented can be easily generalized to the case with a background light. In this case, one has to first numerically compute the steady-state values corresponding to the background light, and then use the analysis with parameters that have been normalized with these steady state values.

In this work we performed mathematical analysis to obtain quantitative and conceptual understanding. We hope that this work will serve as a template to derive more general results in future work, and that it might inspire new experiments to test the Ca^{2+} dynamics. Apart from phototransduction, our analysis might also be applied to study other G-protein coupled signalling cascades, for example, in olfaction [69].

Author contributions

AA performed analysis and generated figures. JR designed the research, performed analysis and wrote the manuscript.

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Parameter	Description	Rod	Cone
ξ	Gain of PDE activation	0.18[34]	0.0007 [34]
$\beta_d\ (s^{-1})$	Dark turnover rate	4.1 [34]	11 [34]
$\mu_{rh}\ (s^{-1})$	Deactivation rate of activated photopigment	28 [34]	70 [34]
$\mu_{pde}\ (s^{-1})$	Deactivation rate of activated PDE	5[34]	37.8[34]
$\mu_{tr} = k_{tr}\ (s^{-1})$	Deactivation rate of activated transducin	23.8 [34]	71 [34]
$K_{ex}\ (\mu M)$	Sensitivity of NCKX exchanger to Ca^{2+}	1.6 [6]	1.6
$K_{ch}\ (\mu M)$	Sensitivity of CNG channels to cGMP	20 [6]	20
n_{ch}	CNG channel cooperativity	2.5 [34]	2.5 [34]
$K_{\alpha}\ (\mu M)$	Cyclase affinity to Ca^{2+}	0.14 [70, 55]	0.14
r_{α}	Ratio of minimal to maximal cyclase activity	0.033 [71, 70]	0.033
n_{α}	Hill coefficient for the cyclase	2 [34]	2 [34]
$f_{ch,ca}$	Fraction of the CNG current carried by Ca^{2+}	0.12 [46]	0.3 [72]
$I_0\ (pA)$	Dark current	15 [34]	15 [34]
$c_{ca,d}\ (\mu M)$	Dark Ca^{2+} concentration	0.3 [34]	0.3 [34]
$c_{cg,d}\ (\mu M)$	Dark cGMP concentration	4 [34]	4 [34]
$V_{os}\ (\mu m^3)$	Outer segment volume	18 [48]	7.2 [73, 74]
$c_{rec}\ (\mu M)$	Recoverin concentration	150 [26]	150
$K_{rec}\ (\mu M)$	Ca^{2+} affinity for recoverin	3 [54]	3
$c_{gcaps}\ (\mu M)$	GCAPs concentration	3 [55]	3
$K_{gcaps}\ (\mu M)$	Ca^{2+} affinity for GCAPs	0.14 [55, 70]	0.14

Table 1: Parameter values for mouse rods and cones. Whenever cone values are not known, we simplify and use the rod values.

Figure 1: **Simulations and analytic results of dim-light responses in a mouse rod.** The normalized current $\hat{i}$ with fast and slow Ca^{2+} kinetics is shown for flashes of light at time $t = 0$ with duration $\Delta t = 0.005s$ (A-B), and light steps with duration $\Delta t = 2s$ (C-D). Light intensities are such that the isomerisations $R_0^* = \kappa \phi \Delta t$ are $R_0^* = 1, 2, 3, 4, 5$ in (A-B), and $R_0^* = 4, 9, 15, 25$ in (C-D). Simulations are performed with Eq. 5 and two Ca^{2+} buffers with low and high affinity. In (A,C) the buffer properties are as specified in Table 1 (recoverin and GCAPs buffers). In (B,D) both buffer concentrations have been augmented by a factor of 10. The value of μ_{ca} shown in the panels is computed with Eq. 6. Analytic results $\hat{i} = R_0^* \hat{i}_{spr}$ are computed with $\hat{i}_{spr}$ from Eq. 16. If not specified otherwise, parameters are from Table 1.

Figure 2: **Simulations and analytic results of dim-light responses in a mouse cone.** The normalized current $\hat{i}$ with fast and slow Ca^{2+} kinetics is shown for flashes of light at time $t = 0$ with duration $\Delta t = 0.005s$ (A-B), and light steps with duration $\Delta t = 1s$ (C-D). Light intensities are such that the isomerisations $R_0^* = \kappa\phi\Delta t$ are $R_0^* = 130, 260, 520, 780$ (A-B) and $R_0^* = 650, 2600, 5200, 9100$ (C-D). Simulations are performed with Eq. 5 and two Ca^{2+} buffers with low and high affinity. In (A,C) the buffer concentrations are as specified in Table 1 (recoverin and GCAPs buffers), in (B,D) both buffer concentrations have been augmented by a factor of 10. The value of μ_{ca} shown in the panels is computed with Eq. 6. Analytic results $\hat{i} = R_0^*\hat{i}_{spr}$ are computed with $\hat{i}_{spr}$ from Eq. 16. If not specified otherwise, parameters are from Table 1.

Figure 3: **Single-photon responses (SPRs) and unitary step responses for rod and cone.** Responses are computed with $\hat{i}_{spr}(t)$ from Eq. 16 and μ_{ca} values depicted in panel (A) for cone, and in panel (B) for rod. Solid lines show WT, dashed lines GCAPs$^{-/-}$ responses (the Ca^{2+} feedback to the cyclase is removed). The cone step responses in (C) have light duration $\Delta t = 1s$, the rod response in (D) have $\Delta t = 2s$.

Figure 4: **Waveform of flash and step responses in cone**. (A) The current waveform of a dim-flash response is obtained by normalizing the SPRs from Fig. 3A with the peak amplitude. (B) For longer step responses, the waveform is obtained by normalizing the responses in Fig. 3C with the intermediate plateau values. (C-D) The waveform of the Ca^{2+} concentration is computed similar to the current waveform using $1 - \hat{c}_a(t)$. The current waveforms (solid lines) from (A-B) for $\mu_{ca} = 10, 20, 50s^{-1}$ are compared to the corresponding Ca^{2+} waveforms (dashed lines). The color coding is as in (A-B).

Figure 5: **Decomposition of the SPR waveform.** The decomposition of the SPR waveform (black line) is computed with Eq. 17. In every panel, the black line is the sum of the colored lines. (A) SPR decomposition for a WT rod with $\mu_{ca} = 50s^{-1}$, (B) GCAPs$^{-/-}$ cone with $\mu_{ca} = 20s^{-1}$, (C) WT rod with $\mu_{ca} = 5s^{-1}$, (D) WT cone with $\mu_{ca} = 20s^{-1}$.

Figure 6: **Phase space for Ca^{2+} oscillations**. (A) Range for μ_{ca} where oscillations occur as a function of $\tilde{n}_{ch}\hat{\alpha}'_0$ for rod (red) and cone (back) (see section 2.2.1 for more details). The blue horizontal line indicates the value $\tilde{n}_{ch}\hat{\alpha}'_0 \approx 4$ computed with parameters from Table 1. (B) Oscillation frequency ω as a function of μ_{ca} for rod and cone. The maximal frequency $\omega_{max} \approx \beta_d \frac{9}{2}$ is achieved for $\mu_{ca} \approx \beta_d 9$.

Figure 7: **Effect of changing the extracellular Ca^{2+} concentration for a cone.** (A) Changes in the dark steady state concentrations of Ca^{2+} (black curve), cGMP (red curve), and dark current (blue curve) when the extracellular Ca^{2+} concentration is altered by a factor of $r_{ca,ex}$. (B) Comparison of the normalized SPR current $\hat{i}_{spr}$ (Eq. 16) for $r_{ca,ex} = 0.1$ (solid lines) and $r_{ca,ex} = 1$ (dashed lines) for various μ_{ca}. The dashed curves are identical to the solid curves in Fig. 3A. (C) The dimensional SPR currents are obtained by multiplying the traces in (B) with the corresponding dark currents $I_d = 3.8 \times 15pA$ ($r_{ca,ex} = 0.1$) and $I_d = 15pA$ ($r_{ca,ex} = 1$). (D) Comparison of the SPR waveforms for $\mu_{ca} = 50s^{-1}$.

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