Age-related changes in the neural mechanics of dynamic auditory attention in time

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29   Abstract

Listening in everyday life requires attention to be deployed dynamically – when listening is expected to

be difficult and when relevant information is expected to occur – to conserve mental resources.

Conserving mental resources may be particularly important for older adults who often experience

difficulties understanding speech. We use electro- and magnetoencephalography to investigate the

neural and behavioral mechanics of dynamic attention regulation during listening and the effects that

aging may have on these. We show that neural alpha oscillatory activity indicates when in time attention

is deployed (Experiment 1) and that deployment depends on listening difficulty (Experiment 2). Older

adults also show successful attention regulation, although younger adults appear to utilize timing

information a bit differently compared to older adults. We further show that the recruited brain regions

differ between age groups. Superior parietal cortex is involved in attention regulation in younger adults,

whereas posterior temporal cortex is more involved in older adults (Experiment 3). This difference in the

sources of alpha activity across age groups was only observed when a task was performed, and not for

alpha activity during resting-state recordings (Experiment S1). In sum, our study suggests that older

adults employ different neural control strategies compared to younger adults to regulate attention in

time under listening challenges.

Keywords: Listening, attention, cognitive control, aging, neural oscillations, alpha power

49   **Significance statement**

Listening requires attention to be deployed dynamically in time to conserve mental resources.

Conserving mental resources may be especially important for older adults who often experience

listening difficulties. We investigate the neural and behavioral mechanics of dynamic attention during

listening in younger and older adults. We show that neural alpha oscillatory activity indicates when in

time attention is deployed and that deployment depends on listening difficulty. Older adults appear to

employ more reactive than proactive listening behavior and recruit different brain regions than younger

adults. Superior parietal cortex is involved in younger adults, whereas posterior temporal cortex in older

adults. In sum, older adults may use different strategies compared to younger adults to regulate

attention in time during challenging listening.

Introduction

Speech is often difficult to understand, either because of situational demands (e.g., background speech),

or because of age-related changes in sensory systems (Pichora-Fuller, 2003; Mattys et al., 2012;

Johnsrude and Rodd, 2016). Degraded speech increases the need to recruit cognitive resources such as

attention, but this is mentally costly (Westbrook and Braver, 2015; Hornsby et al., 2016; Shenhav et al.,

2017) and makes listening effortful (Pichora-Fuller, 2016; Strauss and Francis, 2017; Peelle, 2018;

Herrmann and Johnsrude, 2020). Critically, situational demands vary over time as the intensity and

character of background speech change, and not all words are equally important for a listener to follow

a conversation. Hence, the effort required to comprehend may also fluctuate. A listener could attend

specifically at times when listening is expected to be difficult or when relevant information is expected

to occur in order to reduce experienced effort and conserve mental resources; this makes listening a

temporally dynamic process. The current work explores the neural and behavioral signatures of dynamic

attention during listening and the changes associated with aging.

Electro-/magnetoencephalography (EEG/MEG) measuring neural oscillatory activity in the alpha

(~10 Hz) frequency band provides a unique window on cognition (Klimesch, 1999; Klimesch et al., 2007;

Jensen and Mazaheri, 2010). High alpha power has been associated with the recruitment of cognitive

resources during listening (Adrian, 1944; Foxe et al., 1998; Fu et al., 2001; Palva and Palva, 2011). For

example, alpha power increases when individuals listen actively compared to passively (Dimitrijevic et

al., 2017; Henry et al., 2017) or listen to degraded, difficult-to-understand speech (Wöstmann et al.,

2015). Alpha activity further appears to be sensitive to temporal dynamics of cognitive processing. Alpha

power synchronizes with attended words presented in dichotic speech-listening tasks (Wöstmann et al.,

2016; Tune et al., 2018; Wöstmann et al., 2021) and temporally aligns with an anticipated visual stimulus

(Rohenkohl and Nobre, 2011; Bonnefond and Jensen, 2012; Payne et al., 2013). Here, we focus on how

alpha activity changes over time as individuals direct attention dynamically when key information is

expected to occur during challenging listening.

Older adulthood is associated with reduced cognitive control abilities, including attentional

control (Braver and Barch, 2002; Braver, 2012; Zanto and Gazzaley, 2017). Consistent with age-related

reductions in cognitive control, behavioral performance and attention-related lateralization of alpha

power in visuospatial tasks is reduced in older compared to younger adults (Zanto et al., 2011; Sander

et al., 2012; Hong et al., 2015; Leenders et al., 2018; Dahl et al., 2019). In active listening tasks, alpha

power typically increases relative to baseline (Wöstmann et al., 2015; Dimitrijevic et al., 2017; Henry et

al., 2017), but older adults show weaker power increases (Wöstmann et al., 2015; Rogers et al., 2018)

or even suppression of alpha power compared to younger individuals (Henry et al., 2017; Getzmann et

al., 2020). Moreover, attention-related lateralization of alpha power in auditory spatial tasks appears to

be reduced in older compared to younger adults (Getzmann et al., 2020) and in adults with hearing

impairment compared to those without (Bonacci et al., 2019). However, from these works it is unclear

whether dynamic attending to key points in time during challenging listening is affected by aging.

In the current experiments using EEG (Experiments 1 and 2) and MEG (Experiments 3 and S1),

participants listened to 10-s white noise sounds, detecting a gap target that they were informed

occurred in the first half of the sound, or in the second half. This paradigm allows us to capture neural

activity and behavior as listeners flexibly deploy attention either early or late in a stimulus. We test

whether neural alpha power indexes the dynamic deployment of attention (Experiment 1) and whether

alpha power changes with the degree of expected listening difficulty (Experiment 2). We then investigate

whether dynamic attending during challenging listening, as indexed by alpha power and behavior, differs

between younger and older adults (Experiment 3), and whether any age differences are observed only

when a task is performed, or are also present during resting-state alpha recording (Experiment S1).

General Methods

Participants

In total, 132 male and female adults of varying age participated in the experiments of the current study.

Different participants were recruited for each of the three main experiments and the one supplementary

experiment (see Experiment S1 in the Supplemental Materials). Demographic details are described

below for each experiment individually. Participants reported no neurological disease or hearing

impairment and were naïve to the purpose of the experiment. Participants gave written informed

consent prior to the experiment and were paid for their participation. The study was conducted in

accordance with the Declaration of Helsinki, the Canadian Tri-Council Policy Statement on Ethical

Conduct for Research Involving Humans (TCPS2-2014), and approved by the Nonmedical Research Ethics

Board of the University of Western Ontario (protocol ID: 106570).

Stimulation apparatus

All EEG sessions (Experiments 1 and 2) were carried out in a sound-attenuating booth. Sounds were

presented via Sennheiser (HD 25-SP II) headphones and a Steinberg UR22 (Steinberg Media

Technologies) external sound card. Stimulation was controlled by a PC (Windows 7) running

Psychtoolbox in MATLAB (MathWorks Inc.).

All MEG sessions (Experiments 3 and S1) were carried out in an electromagnetically shielded,

sound-attenuating room (Vacuumschmelze, Hanau). Sounds were presented via in-ear phones and the

stimulation was controlled by a PC (Windows XP) running Psychtoolbox in MATLAB.

Acoustic stimulation and procedure

At the beginning of Experiments 1-3, each participant's hearing threshold was measured for a white

noise stimulus using a methods of limits procedure, which we have described in detail in previous work

(Herrmann and Johnsrude, 2018). Acoustic stimuli were presented at 50 dB (Experiments 1 and 2) or 45

dB (Experiment 3) above the individual's hearing threshold (sensation level).

Acoustic stimuli during the main experimental procedures were 10-s white noise sounds that

each contained one short gap (Figure 1A). The participants' task was to press a button as soon as they

detected the gap (Henry and Obleser, 2012; Henry et al., 2014, 2016; Henry et al., 2017). The white

noise 0.4 s prior to and 0.1 s after a gap was identical for each sound, whereas the remainder of the 10-

s white noise differed from trial to trial. This ensured that the probability of detecting a gap would be

unaffected by trial-by-trial acoustic variations just prior and subsequent to a gap. Gap duration was

titrated for each individual to approximately 70-80% detected gaps in training blocks (N=2-4; ~2.5 min

each) prior to the main experiment.

For the main experiment, the gap occurred within a 2.5-s window either within the first half

(1.8–4.3 s) or within the second half (6.3–8.8 s) of the 10-s white-noise sound (Figure 1A). Sounds were

separated by a 2-s inter-stimulus interval. Participants were informed about whether the gap would

occur in the first or the second half of the sound and this expectation was never violated. Participants

could thus orient their attention in time, but they did not know exactly when, within the cued half of the

sound, the gap would occur. Trials in which the gap occurred in the first half and trials in which the gap

occurred in the second half of the sound were presented in separate blocks. The number of blocks and

the number of trials per block are described below for each experiment separately.

Behavioral data analysis

For each sound trial, as long as the gap has not yet occurred, the instantaneous probability of the gap's

occurrence within the cued time window (first half; second half) increases monotonically with the

passage of time. This is the "hazard rate" (Niemi and Näätänen, 1981; Nobre et al., 2007; Nobre and van

Ede, 2018). Response times are expected to be faster for gaps occurring late compared to early within a

cued time window (Niemi and Näätänen, 1981; Nobre et al., 2007). This "hazard-rate effect" indicates

successful allocation of attention in time (Nobre et al., 2007). Analyzing behavioral data as a function of

time within a cued time window allows us to capture whether individuals orient attention in time during

listening.

A gap was considered detected (i.e., a hit) if a response was made between 0.1 and 1.2 s after

gap onset, and undetected (i.e., a miss) if no button was pressed within that time window. In order to

investigate the effect of the passage of time on behavioral performance, behavioral data were analyzed

as a function of the gap time within a cued sound half (ranging from 0 to 2.5 s). In detail, hit rates were

analyzed by calculating a logistic regression (generalized linear model with a binomial/logit link function;

Tune et al., 2021) that relates single-trial responses to gap times. For the response times (hazard-rate

effect; Niemi and Näätänen, 1981; Nobre et al., 2007), a linear function was fit to relate single-trial

response times to gap times. The logistic regression (hit rate) and linear function (response time) were

fit separately for each participant and condition (e.g., participants cued to the first vs second half of the

sound). The slope of the fits describes the relation between hit rate / response time and gap time, and

was used as the dependent measure.

EEG/MEG recordings and preprocessing

Details about EEG and MEG recordings and preprocessing are provided for each experiment below. In

short, EEG (16 electrodes) and MEG (204 channels) data were high-pass filtered at 0.7 Hz, low-pass

filtered at ~30 Hz, and divided into epochs ranging from −2 to 12 s time-locked to sound onset.

Independent components analysis (ICA; Makeig et al., 1996) was used to identify and suppress activity

related to blinks, horizontal eye movements, and the heart.

Wavelet analysis and alpha power

Wavelet coefficients were calculated by convolving single-trial data epochs (-2 to 12 s) with Morlet

wavelets. For each participant, trial, and channel, wavelet coefficients were calculated for frequencies

ranging from 1 to 20 Hz (in steps of 0.5 for Experiments 1 and 2; in steps of 1 Hz for Experiment 3) and

time points ranging from −1.5 to 10 s (in steps of 0.0156 s for Experiments 1 and 2; in steps of 0.024 s

for Experiment 3). Single-trial time-frequency power representations were obtained by squaring the

magnitude of the complex wavelet coefficients. Time-frequency power was averaged across trials for

each cue condition (first half; second half) and baseline corrected using relative change (Capilla et al.,

2014; Wilsch et al., 2015; Dimitrijevic et al., 2017; Henry et al., 2017; Fiedler et al., 2021). That is, the

mean power preceding sound onset (−1.5 to −0.2 s) was subtracted from the power values at each time

point. The resulting values were divided by the mean power in the pre-sound onset time window (−1.5

to −0.2 s).

Auditory alpha activity often covers a frequency band below 10 Hz (Niedermeyer, 1990; Tiihonen

et al., 1991; Lehtelä et al., 1997; Obleser et al., 2012; Billig et al., 2019) compared to the traditional

occipital alpha activity peaking at about 10 Hz (Berger, 1929). Indeed, in the experiments of the current

study, the frequency of alpha activity was significantly lower than 10 Hz (Figure S1). Alpha power was

thus averaged across frequencies between 8 and 10 Hz. This lower frequency band also avoids

contributions of power suppressions to the average that were occasionally present at higher frequencies

(e.g., Figures 4A, 6A/B; small variations in the selected frequency band do not affect the current results).

In order to investigate whether alpha power is sensitive to participants attending to the first

versus second half of the sound, we averaged alpha power in the 0.8-s time interval prior to the 2.5 s

during which a gap could occur in the two cue conditions (first interval: 1–1.8 s; second interval: 5.5–

6.3 s). Using alpha power as a dependent measure, an rmANOVA was calculated including the within-

participants factors Time Interval (first interval; second interval) and Cue (first half; second half). For

Experiment 2, the within-participants factor Task Difficulty (easy; difficult) was additionally included. For

Experiment 3, we included the additional between-participants factor Age Group (younger; older).

Statistical analysis

The experiments reported here were not preregistered. Experimental manipulations were within-

participants factors and age group in Experiments 3 and S1 was a between-participants factor.

Differences between experimental conditions were thus assessed using one-sample t-tests, paired-

samples t-tests, and repeated-measures ANOVAs (rmANOVAs). Age-group differences in Experiment 3

(and Experiment S1) were assessed using a between-participants factor in rmANOVAs or independent-

samples t-tests. Reporting of statistical results includes test statistic, degrees of freedom, significance

level, and effect size. Details about statistical analyses are provided for each experiment separately

below. Throughout the manuscript, effect sizes are provided as partial eta squared (η^2_p) for ANOVAs and

Cohen's d for t-tests.

209   **Experiment 1: Investigation of dynamic attention in time during listening**

Methods

Participants

Twenty-two participants were recruited for Experiment 1 (age range: 18–31 years; median: 20 years; 14

females and 8 males). For two participants, data from two blocks were excluded because recording of

behavioral responses malfunctioned.

Procedures

Participants listened to 10-s white-noise sounds in six blocks, each containing 40 trials (N=50 for eight

participants). Within each block, a gap could occur at one of 40 (50) uniformly spaced times during a 2.5

s window, randomly drawn without replacement. In three of the six blocks, the gap always occurred

within a 2.5-s window in the first half (1.8–4.3 s), whereas in the other three blocks, the gap always

occurred within the second half (6.3–8.8 s) of the 10-s white-noise sound (Figure 1A). Hence, participants

were presented with 120 (150) trials per cue condition. For each block, participants were cued as to

whether the gap would occur in the first or the second half of the sound. Blocks with gaps occurring in

the first versus second half of the sound alternated within an experimental session and the starting

condition alternated across participants.

Behavioral analysis

A dependent samples t-test was used to compare overall hit rate and response times between the two

cue conditions (first half; second half). The relationship between gap time and behavioral performance

was assessed by comparing hit rate/response time slopes against zero using a one-sample t-test. A

dependent-samples t-test was calculated to compare slopes between cue conditions.

EEG recordings and preprocessing

EEG was recorded at a 1024-Hz sampling rate from 16 electrodes (Ag/Ag–Cl-electrodes; 10-20

placement) and additionally from the left and right mastoids (BioSemi, Amsterdam, The Netherlands;

208 Hz low-pass filter). Electrodes were referenced online to a monopolar reference feedback loop

connecting a driven passive sensor and a common mode sense active sensor, both located posterior on

the scalp.

Offline data analysis was carried out using MATLAB software (v7.14; MathWorks, Inc.). Line noise

(60 Hz) was suppressed using an elliptic filter. Data were re-referenced to the average mastoids, high-

pass filtered at a cutoff of 0.7 Hz (2449 points, Hann window), and low-pass filtered at a cutoff of 30 Hz

(111 points, Hann window). Data were divided into epochs ranging from −2 to 12 s (time-locked to sound

onset) and ICA (runica method, Makeig et al., 1996; logistic infomax algorithm, Bell and Sejnowski, 1995;

Fieldtrip implementation Oostenveld et al., 2011) was used to identify and suppress activity related to

blinks and horizontal eye movements. Epochs that exceeded a signal change of more than 250 μV for

any electrode following ICA were excluded from analyses.

Time-frequency power was calculated for each cue condition (first half; second half) and alpha-

power time courses were calculated as the mean power across the 8–10 Hz frequencies (see General

Methods). Alpha activity was averaged across a parietal electrode cluster (Pz, P4, P3). We averaged alpha

power in the 0.8-s time interval prior to the 2.5 s during which a gap could occur in the two cue

conditions (first interval: 1–1.8 s; second interval: 5.5–6.3 s). An rmANOVA was calculated using alpha

power as the dependent measure and the within-participants factors Time Interval (first interval; second

interval) and Cue (first half; second half).

Results and discussion

Gap-detection hit rates were generally higher (t_{21} = 3.045, p = 0.006, d = 0.649) and response times generally faster (t_{21} = 2.237, p = 0.036, d = 0.477) for gaps occurring in the first compared to the second half of the sound (Figure 1B). This suggests that focusing attention to later parts of the sound is more difficult than focusing on earlier parts. Listeners may struggle more to precisely focus attention when gaps occur in the second half of the sound due to well-known higher variability in time-interval estimations for longer relative to shorter intervals (Weber's law; Gibbon, 1977; Buhusi and Meck, 2005; Grondin, 2014).

Figure 1: Stimulus representation and behavioral performance for Experiment 1. A: Participants were presented with 10-s white noises that contained one gap. The gap occurred within a 2.5-s window either within the first half (1.8–4.3 s) or within the second half (6.3–8.8 s) of the noise (colored dashed lines). Participants were cued as to whether the gap would occur in the first or the second half of the sound, allowing them to orient their attention in time. Participants did not know exactly when, within the cued half of the sound, the gap would occur. B: Predicted hit rates and response times from logistic and linear fits, respectively, as a function of gap occurrence within the cued 2.5-s window. The x-axis reflects the gap time relative to the onset of the cued time window (1.8 s and 6.3 s for first half and second half, respectively). Slopes from logistic (hit rate) and linear (response time) fits are plotted as bar graphs and individual data points. Error bars and shadings reflect the standard error of the mean. *p ≤ 0.05, n.s. – not significant.

Critically, gap-detection hit rates were higher (t_{21} = 3.746, p = 0.001, d = 0.799) and response times faster (t_{21} = 7.115, p = 5.11 × 10^{-7}, d = 1.517) for gaps that occurred later compared to earlier within the cued 2.5-s window (averaged across attention conditions). This was true regardless of whether that window was in the first or second half of the trial (see slopes in Figure 1B). The faster response times for gaps occurring later within a cued half indicate that participants successfully oriented attention in time (hazard-rate effect; Niemi and Näätänen, 1981; Nobre et al., 2007). This response-time effect was smaller when participants attended to the second compared to the first half of the sound (t_{21} = 4.093, p = 5.2 × 10^{-4}, d = 0.873). The reduced hazard-rate effect suggests that individuals' estimation

267 of when a gap may occur is reduced when gaps occur in the second compared to the first half of the

268 sound. This, again, is consistent with higher variability in time estimations for longer relative to shorter

269 intervals (Gibbon, 1977; Buhusi and Meck, 2005; Grondin, 2014).

Figure 2: Sensitivity of alpha power to attentive listening in time. **A:** Time-frequency power (averaged across parietal electrodes; dashed lines mark the 2.5-s windows [gap occurrence]). **B:** Alpha-power (8–10 Hz) time course for the two cue conditions (first half; second half). Colored lines on the x-axis mark the 2.5-s windows (gap occurrence). Mean alpha power in the 0.8-s time interval prior to the 2.5-s gap window (bottom). **C:** Alpha-power time courses sorted by gap occurrence. The dashed line indicates the gap onset. Error bars and shadings reflect the standard error of the mean. *p ≤ 0.05, n.s. – not significant.

Alpha power was sensitive to whether participants attended to the first versus second half of the

sound: alpha power increased for longer when participants knew the gap would occur later, that is, in

the second compared to the first half (Figure 2A/B). For the rmANOVA, we observed a Time Interval ×

Cue interaction ($F_{1,21}$ = 14.389, p = 0.001, η_p^2 = 0.407): Alpha power was larger in the first interval (1−1.8

s) compared to the second interval (5.5–6.3 s) when participants were cued to the first half ($F_{1,21}$ = 7.549,

p = 0.012, η_p^2 = 0.264), but alpha power was larger in the second interval (5.5–6.3 s) compared to the

first interval (1−1.8 s) when participants were cued to the second half of the sound ($F_{1,21}$ = 13.176, p =

0.002, η_p^2 = 0.386; Figure 2B, bottom). In fact, alpha power increased throughout a trial up to gap

occurrence and decreased thereafter (Figure 2C).

The results from Experiment 1 demonstrate that individuals attend dynamically in time during

listening according to when they expect a target, and alpha power indicates when in time individuals

listen attentively. Our core paradigm is thus suitable for the study of attention regulation in time during

listening.

Experiment 2: Investigation of dynamic attention regulation under different listening difficulty

Next, we turned to the observation that older adults often experience listening challenges in their

everyday lives (Gatehouse and Noble, 2004; Pichora-Fuller et al., 2016; Strauss and Francis, 2017; Peelle,

2018). Individuals can conserve mental resources associated with listening challenges by regulating how

much attention is deployed based on the expected difficulty of a listening situation (Brehm and Self,

1989; Richter et al., 2016; Herrmann and Johnsrude, 2020). Alpha power should be sensitive to such

regulations of attention based on expected listening difficult if it is to be useful for the study of dynamic

attention. Experiment 2 aims to investigate how cuing a listener to attend to specific points in time and

task difficulty affect behavior and neural alpha activity.

Methods

Participants

Experiment 2 included 20 younger adults (age range: 17–30 years; median: 18; 16 female and 4 males).

Procedures

Similar to Experiment 1, we manipulated when a gap occurred (first half; second half), and the cue given

prior to a block of trials, in order to manipulate attention in time. In addition, task difficulty was

manipulated by changing the duration of the gap (Figure 3A). The estimated gap-duration threshold

from the training blocks was used for difficult, short-duration trials (as in Experiment 1), whereas three

times the estimated threshold was used for easy, long-duration trials. The different cue (first half; second

half) and task-difficulty (easy; difficult) trials were presented in separate blocks. Participants were cued

prior to each block whether the gap would occur in the first or the second half of the sound, and whether

gap detection would be easy or difficult, and these expectations were never violated. Participants thus

had prior knowledge about which sound conditions they would encounter so that they could regulate

their attention. Participants listened to 35 trials per block and each of the four block types was presented

twice. Within each block, a gap could occur at one of 35 uniformly spaced times during the cued 2.5 s

window (cued to first half: 1.8-4.3 s; cued to second half: 6.3-8.8 s), randomly drawn without

replacement. Block order was organized such that cue conditions alternated (first half; second half),

whereas task-difficulty conditions (easy; difficult) were presented in two consecutive blocks and

alternated to create a balanced design. Starting conditions alternated across participants.

Behavioral data analysis

A rmANOVA was used to compare overall hit rate and response times between the two cue conditions

(first half; second half) and the two task-difficulty conditions (easy; difficult). The relationship between

gap time and behavioral performance was assessed by comparing hit rate/response time slopes against

zero using a one-sample t-test. A rmANOVA and t-tests were used to compare slopes between the cue

conditions (first half; second half) and the task-difficulty conditions (easy; difficult).

EEG recording and analysis

EEG recording and preprocessing was conducted as for Experiment 1.

Alpha power (8–10 Hz) was averaged in the 0.8-s time interval prior to the cued 2.5-s time

window during which a gap could occur in the two cue conditions (first interval: 1–1.8 s; second interval:

5.5–6.3 s), separately for the two cue and task-difficulty conditions. An rmANOVA was calculated using

alpha power as the dependent measure and the within-participants factors Time Interval (first interval;

second interval), Cue (first half; second half), and Task Difficulty (easy; difficult).

Results and discussion

Figure 3B depicts the behavioral results for Experiment 2. Hit rates were overall higher ($F_{1,19}$ = 63.007, p

= 1.89×10^{-7}, η_p^2 = 0.768) and response times faster ($F_{1,19}$ = 262.594, p = 1.4×10^{-12}, η_p^2 = 0.933) for easy

compared to difficult trials, but did not differ between cue conditions (p > 0.25).

Because hit rates for easy trials were at ceiling, the relationship between hit rate and gap time

was not analyzed for easy trials. For difficult trials (short gap), hit rates increased with increasing gap

time within the cued 2.5-s windows (t_{19} = 3.598, p = 0.002, d = 0.804; averaged across conditions; slopes

in Figure 3B). There was no difference between attention conditions (p > 0.2).

Figure 3: Stimulus representation and behavioral performance for Experiment 2. A: Schematic representation of the gap duration for easy and difficult trials (long and short gap durations, respectively). The duration of the short gap was titrated for each individual to approximately 80% detection rate. The duration of the long gap was three times the duration of the short gap. **B:** Predicted hit rates and response times from logistic and linear fits, respectively, as a function of gap occurrence within the 2.5-s window, for both cue (first half; second half) and task-difficulty (easy [dashed]; difficult [solid]) conditions. The x-axis reflects the gap time relative to the onset of the cued time window (1.8 s and 6.3 s for first half and second half, respectively). Slopes from logistic (hit rate) and linear (response time) fits are plotted on the right. Slope for hit rates from the easy condition were less reliable due to ceiling effects; they are thus not displayed. Error bars and shadings reflect the standard error of the mean. *$p \leq 0.05$, n.s. – not significant.

Response times decreased with increasing gap time within the cued 2.5-s window (i.e., hazard-
rate effect: $t_{19} = 7.698$, $p = 2.96 \times 10^{-7}$, $d = 1.721$; averaged across conditions; Figure 3B), but this effect
was larger when participants attended to the first half compared to the second half of the noise ($F_{1,19} =$
25.874, $p = 6.55 \times 10^{-5}$, $\eta_p^2 = 0.577$). The hazard-rate effect was unaffected by task difficulty ($p > 0.15$),
suggesting that participants orient attention in time to the same extent for easy and difficult trials (Figure
3B).

Figure 4: Sensitivity of alpha power to attentional orienting and task difficulty during listening. A: Time-frequency (averaged across parietal electrodes) power representations for each of the four Cue × Task Difficulty conditions. **B:** Alpha power (8–10 Hz) time courses and topographical distributions. **C:** Mean alpha power in the 0.8-s time interval prior to the 2.5-s gap windows. Error bars and shadings reflect the standard error of the mean. *$p \leq 0.05$, n.s. – not significant.

Time-frequency power representations and alpha power time courses are depicted in Figure 4A
and B, respectively. The rmANOVA for alpha power revealed a Time Interval × Cue interaction ($F_{1,19} =$
21.001, $p = 2.03 \times 10^{-4}$, $\eta_p^2 = 0.265$). Alpha power was larger in the first interval (1–1.8 s) compared to
the second interval (5.5–6.3 s) when participants were cued to the first half ($F_{1,19} = 7.697$, $p = 0.012$, η_p^2

= 0.288), but alpha power was larger in the second interval (5.5–6.3 s) compared to the first interval (1–

1.8 s) when participants were cued to the second half ($F_{1,19}$ = 21.556, p = 1.8^{e-4}, η_p^2 = 0.532; Figure 4C).

These results replicate the results from Experiment 1 by showing that alpha power indicates when in

time individuals listen attentively.

In addition, the Time Interval × Cue × Task Difficulty interaction was marginally significant ($F_{1,19}$

= 4.022, p = 0.059, η_p^2 = 0.175): we conducted an exploratory analysis to understand this marginal

interaction in more detail. Separately for each cue condition (first half; second half), a rmANOVA with

Time Interval (first interval: 1–1.8 s; second interval: 5.5–6.3 s) and Task Difficulty (easy; difficult) factors

was conducted. When participants were cued to the first half of the sound, alpha power was larger for

difficult compared to easy trials (effect of Task Difficulty: $F_{1,19}$ = 4.980, p = 0.038, η_p^2 = 0.208), but there

was no Time Interval × Task Difficulty interaction (p = 0.204). In contrast, when participants were cued

to the second half of the sound, alpha power increased over time in both difficulty conditions, but the

increase was steeper for difficult compared to easy trials (Time Interval × Task Difficulty interaction: $F_{1,19}$

= 4.638, p = 0.044, η_p^2 = 0.196).

Experiment 2 shows that alpha power increased with increasing task difficulty when individuals

attended to the first half of the sound. When participants attended to the second half of the sound,

alpha power increased over time for both easy- and difficult-to-detect gaps, but the rate of alpha power

increase over time was larger. That task difficult had a clearer impact on alpha power when gaps

occurred in the first compared to the second half of the sound may be related to overall difficulty

differences: Gap detection appears to be easier when gaps occur in the first half compared to the second

half of a sound (e.g., Figure 1B, 5A), possibly due to higher variability in time estimations for longer

compared to shorter intervals (Gibbon, 1977; Wearden, 2003; Buhusi and Meck, 2005; Grondin, 2014).

Alpha power may thus increase when participants attend to the second half of the sound because

orienting and maintaining attention over a longer period may be difficult, independent of the

experimentally manipulated difficulty (gap duration).

The results from Experiment 2, together with those from Experiment 1, indicate that alpha power

is sensitive both to 'when' an individual is listening, as well as to 'how hard' they are listening (how

effortful it is). Alpha power may therefore be a useful way to measure whether younger and older adults

differ in how they direct attention to points in time when key information is expected to occur during

challenging listening.

Experiment 3: Assessing age differences in dynamic attention regulation in time

Experiment 3 aims to investigate whether behavioral and neural indices of attention regulation in time

differ between younger and older adults, and to characterize the brain regions underlying such attention

regulation. We recorded MEG in younger and older adults using the same experimental procedures as

those in Experiment 1 (Figure 1A).

Methods

Participants

Twenty-five younger (age range: 20–33 years; median: 26 years; 15 females and 10 males) and twenty-

seven older adults (age range: 54–72 years; median: 63 years; 13 female and 14 males) participated in

Experiment 3.

Procedures

The same experimental procedures as those in Experiment 1 were used (Figure 1A).

Behavioral data analysis

A rmANOVA was used to compare overall hit rate and response times between the two cue conditions

(within-participants factor: first half; second half) and the two age groups (between-participants factor:

younger; older). The relationship between gap time and behavioral performance was assessed by

comparing hit rate/response time slopes against zero using a one-sample t-test. A rmANOVA and t-tests

were used to compare slopes between cue conditions (first half; second half) and age groups (younger;

older).

MEG recordings and analysis

Magnetoencephalographic data were recorded using a 306-channel Neuromag Vectorview MEG (Elekta;

sampling rate: 1000 Hz, filter: DC–330 Hz) at the Max Planck Institute for Human Cognitive and Brain

Sciences in Leipzig, Germany. The signal space separation (SSS) method was used to suppress external

interference, interpolate bad channels, and transform individual data to a common sensor space. The

common sensor space enables comparison of topographical distributions across participants (Taulu et

al., 2004; Taulu et al., 2005). We focused on the 204 orthogonal planar gradiometers in 102 locations,

because they are most sensitive to magnetic fields originating from sources directly below them

(Hämäläinen et al., 1993). Note that the information in magnetometers and gradiometers after SSS

correction carry redundant information and thus no information is lost by focusing on gradiometers

(Garcés et al., 2017; Herrmann et al., 2018).

Data were high-pass filtered (0.7 Hz; 2391 points, Hann window), low-pass filtered (33.3 Hz, 101

points, Hann window), down-sampled to 500 Hz, and divided into epochs ranging from −2 s to 12 s time

locked to sound onset. Independent components analysis (Makeig et al., 1996; Oostenveld et al., 2011)

was used to remove noisy channels and activity related to blinks, eye movements, and the heart. Epochs

comprising a signal change larger than 300 pT/m in any gradiometer channel following ICA were

excluded.

For each participant, time-frequency power was calculated for each cue condition (first half;

second half). Alpha-power time courses were calculated by averaging power across the 8 to 10 Hz

frequency window. Alpha power (8–10 Hz) was averaged in the 0.8-s time interval prior to the 2.5 s

during which a gap could occur in the two cue conditions (first interval: 1–1.8 s; second interval: 5.5–6.3

s). A rmANOVA with within-participants factors Time Interval (first interval; second interval) and Cue

(first half; second half), and the between-participants factor Age Group (younger; older) was calculated.

MEG source reconstruction

Anatomically constrained source localization was used in order to identify the neural sources underlying

alpha power. Individual T1-weighted MR images (3T Magnetom Trio, Siemens AG, Germany) were used

to construct inner-skull surfaces (volume conductor) and mid-gray matter cortical surfaces (source

model; Freesurfer and MNE software). No MRI scan was available for one older participant and data

from this person were thus not considered for source analyses and related statistical analyses. The MR

and the MEG coordinate systems were co-registered using MNE software which included an automated

and iterative procedure that fitted the >300 digitized head surface points (Polhemus FASTRAK 3D

digitizer) to the MR reconstructed head surface (Besl and McKay, 1992). For each participant, a boundary

element model (inner skull) was constructed using MNE software and a lead field was calculated using

Fieldtrip (Nolte, 2003).

Source reconstructions for time-frequency representations were calculated using dynamic

imaging of coherent sources (DICS; Gross et al., 2001) with custom MATLAB scripts. DICS is a

beamforming technique that involves estimating a spatial filter at each source location. The cross-

spectral density matrix was calculated from the complex wavelet coefficients of all trials in the 8–10 Hz

frequency window and 0.8–9.2 s time window, and used to estimate real-numbered spatial filters (using

the dominant direction; Gross et al., 2001). The 0.8–9.2 s time window was chosen to ensure that power

related to onset or offset responses do not influence the filter calculation. Single-trial wavelet

coefficients were projected into source space using these filters and power time courses were calculated

similar to the sensor space analysis.

Individual cortical representations were transformed to a common coordinate system (Fischl et

al., 1999b). Neural activity in source space was spatially smoothed across the surface using an

approximation to a 6-mm FWHM Gaussian kernel (Han et al., 2006). Neural activity maps were finally

morphed to the standard Freesurfer cortical surface for display purposes (Fischl et al., 1999a).

Statistical analysis of source data

Analysis of age differences in spatial location of alpha activity focused on a pre-gap time window

independent of cue conditions. To this end, alpha power was averaged in the -0.8 to -0.2 s time window

prior to each trial's specific gap onset (-0.2 was chosen to avoid that gap-related activity influences pre-

gap alpha power). Age-differences in spatial configuration of alpha activity were assessed by calculating

for each participant and brain hemisphere the 3D coordinate at which pre-gap alpha power was

maximal. Independent-samples t-tests were used to compare the x, y, and z coordinate between age

groups.

Analysis of inter-subject correlation of alpha power maps was additionally used to examine age

differences in spatial configuration of alpha activity. Each participant's spatial map of pre-gap alpha

power was separately correlated with the spatial map of every other participant (vertices were used as

samples). For each participant, this resulted in 50 correlation values. The 50 correlation values were

categorized into two categories: correlations with members of the same age group (within) and

correlations with members of the other age group (between). For each participant, the average

correlation value was calculated for each of the two categories. This resulted in two mean correlation

values for each participant, reflecting the degree of similarity of the activation map to individuals within

the same versus the other age group. If spatial maps differ between age groups, we would expect larger

correlations with within-group than between-group members. We used independent-samples t-tests to

test this.

457   Previous work suggests task-related alpha activity originates from sensory cortices and parietal

cortex (Tuladhar et al., 2007; van Dijk et al., 2008; Müller et al., 2015; Wöstmann et al., 2016; Tune et

al., 2018). In order to analyze age differences in attentional modulation of alpha power, we used

Glasser's anatomical parcellation of the cortical surface (Glasser et al., 2016) to obtain vertices for

bilateral superior temporal cortex (STC) and bilateral superior parietal cortex (SPC; Figure 6). Alpha

power was averaged within each region, resulting in region-specific alpha-power time courses. Alpha

power was averaged in the 0.8-s interval prior to the 2.5 s during which a gap could occur (first interval:

1–1.8 s; second interval: 5.5–6.3 s). An rmANOVA was calculated using the within-participants factors

Time Interval (first interval; second interval), Cue (first half; second half), and Region (STC, SPC), and the

between-participants factor Age Group (younger; older).

Results and discussion

Age differences in behavioural accuracy but not attentional orienting

Analysis of hit rates revealed no overall difference between age groups ($F_{1,50}$ = 1.457, p = 0.233, η_p^2 =

0.028). Gap-detection hit rates were generally higher for gaps occurring in the first compared to the

second half of the sound ($F_{1,50}$ = 8.312, p = 0.006, η_p^2 = 0.143), as in Experiment 1, perhaps because

focusing attention on later parts of the sound is more difficult than focusing on earlier parts.

473   Critically, hit rates increased with increasing passage of time within the cued 2.5 s window for

474   younger people (t_{24} = 3.467, p = 0.002, d = 0.693), but decreased (numerically) for older people (t_{26} = -

475   0.187, p = 0.853, d = 0.036) as indicated by the age-group difference between slopes ($F_{1,50}$ = 4.817, p =

476   0.033, η_p^2 = 0.088; Figure 5A).

Figure 5: Behavioral results for younger and older adults. Predicted hit rates and response times from logistic and linear fits, respectively, as a function of gap occurrence within the cued 2.5-s window. The x-axis in panels A and B reflects the gap time relative to the onset of the cued time window (1.8 s and 6.3 s for first half and second half, respectively). Error bars and shadings reflect the standard error of the mean. *p ≤ 0.05, n.s. − not significant.

Analysis of response times revealed no overall difference between age groups ($F_{1,50}$ = 0.005, p = 0.944, η_p^2 < 0.001). Response times decreased with increasing gap time within a cued 2.5-s time window (i.e., hazard-rate effect; t_{51} = 6.035, p = 1.81 × 10^{-6}, d = 0.837; average across cue conditions; Figure 5B). There was no effect of age group or interactions involving age groups on response times, although there was a trend towards a larger hazard-rate effect when younger adults were cued to the first half of the sound compared to the second half (t_{24} = 1.792, p = 0.086, d = 0.358; as for Experiment 1; Figure 1B), whereas the hazard rate effect did not differ between cue conditions for older adults (t_{24} = 0.131, p = 0.896, d = 0.025).

In sum, there were no overall differences in hit rates or response times between younger and older adults due to the titration of the gap duration to achieve a hit rate of ~80%. Older adults required the gap to be longer compared to younger adults (t_{50} = 4.282, p = 8.38 × 10^{-5}, d = 1.189) in order to achieve overall similar behavior, consistent with previous gap-detection observations (Snell, 1997; Strouse et al., 1998; Humes et al., 2009; Fitzgibbons and Gordon-Salant, 2010). Response-time data indicate that both younger and older adults successfully oriented attention in time during listening, although there was some indication that younger adults may utilize timing information a bit differently (trending slope differences) compared to older adults. A different picture emerged for hit rates: Younger individuals detected more gaps when they occurred later compared to earlier within a cued sound half,

whereas older individuals detected fewer, potentially suggesting age differences in cognitive control

processes (discussed in detail below).

Younger and older adults show attention-related alpha power modulations

MEG data were first analyzed in sensor space to examine whether MEG alpha power is sensitive to when

participants attend (Figure 6A-D). As for Experiments 1 and 2, the Time Interval × Cue interaction ($F_{1,50}$

= 14.994, p = 3.14 × 10^{-4}, η_p^2 = 0.231) showed that alpha power was larger in the first interval (1-1.8 s)

compared to the second interval (5.5-6.3 s) when participants were cued to the first half ($F_{1,51}$ = 10.646,

p = 0.002, η_p^2 = 0.173), whereas alpha power was larger in the second compared to the first interval

when participants were cued to the second half ($F_{1,51}$ = 12.604, p = 8.4 × 10^{-4}, η_p^2 = 0.198; Figure 6C,D).

This interaction indicates that alpha power was sensitive to whether participants attended to the first

versus second half of the sound.

Figure 6: Effect of age group on listening-related alpha power. A: Time-frequency power (averaged across channels; dashed lines mark the 2.5-s gap window). **B:** Alpha-power (8–10 Hz) time courses for both cue

conditions (first half; second half). Colored lines on the x-axis mark the 2.5-s gap window. Topographies and averaged alpha power are shown for the 0.8-s time interval prior to the 2.5 s during which a gap could occur (first interval: 1–1.8 s; second interval: 5.5–6.3 s). The interaction was significant in younger and older adults. **C:** Source localization of alpha power for both time intervals and age groups. Error bars and shadings reflect the standard error of the mean. *p ≤ 0.05.

We also observed an Cue × Age Group interaction ($F_{1,50}$ = 5.240, p = 0.026, η_p^2 = 0.095): Averaged

across the two analysis time intervals (first and second interval), alpha power was numerically larger for

younger (p = 0.16) but smaller for older adults (p = 0.085) when they were cued to the first compared

to the second half of the sound (Figure 6C/D, right). None of the other effects were significant.

Age-differences in spatial distribution of alpha activity

Analyses described in the previous section were based on activity at MEG sensors, but this potentially

reflects the summed activity from distinct sources (Hämäläinen et al., 1993; Hämäläinen and Hari, 2002).

To gain spatial specificity, we calculated source localizations of alpha power. For younger adults, alpha

power was strongest in superior temporal cortex and superior parietal cortex (Figure 6E). For older

adults, alpha activity was strongest in superior temporal cortex and posterior temporal cortex, and

appeared weaker in superior parietal cortex (Figure 6F; see also Figure S2).

Figure 7: Age-related differences in spatial configuration underlying alpha power. A: Spatial coordinates of alpha power activation peaks for the left (LH) and right hemisphere (RH). Data on the right reflect the mean location on the x-axis (left-right) and z-axis (ventral-dorsal). Activation maxima were more ventro-lateral in older compared to younger adults. **B:** Pair-wise correlation of spatial maps of alpha power among all participants. Correlations were higher among participants from the same age group (within) than with members from the other age group (between), for both younger and older adults. Error bars reflect the standard error of the mean. *p ≤ 0.05, # ≤ 0.1

The analysis of age-group differences in the spatial configuration of alpha power revealed that

peak alpha power was consistently more ventro-lateral in older compared to younger adults (Figure 7A;

x-axis of left hemisphere: t_{49} = 2.833, p = 0.007, d = 0.794; x-axis of right hemisphere: t_{49} = 1.880, p =

0.066, d = 0.527; z-axis of left hemisphere: t_{49} = 3.367, p = 0.002, d = 0.943; z-axis of right hemisphere:

t_{49} = 2.420, p = 0.019, d = 0.678).

Correlations of activation maps among participants further highlight age differences in the spatial

configuration of brain activations: Correlations of spatial alpha-power maps were larger among

members of the same age group (within) compared to members of the other age group (between; Figure

7B; younger adults: t_{24} = 2.812, p = 0.01, d = 0.562; older adults: t_{25} = 3.243, p = 0.003, d = 0.636). These

results suggest that the source configuration underlying listening-related alpha activity differs between

younger and older adults.

In Experiment S1 (see Supplementary Materials), we further show that alpha activity during

active listening (i.e., when there is a task) originates from spatially distinct brain regions compared to

the traditional resting-state alpha activity originating from occipital cortex (Figure S3). This suggests that

there are multiple alpha oscillators in the brain (cf., Başar et al., 1997; Klimesch, 1999; Bollimunta et al.,

2008; van Dijk et al., 2008; Wöstmann et al., 2020). In contrast to alpha activity during active listening,

the sources underlying resting-state alpha activity do not differ between younger and older adults

(Supplementary Materials), suggesting age-specific changes in the listening-related alpha oscillator.

Attentional modulation of alpha power in superior parietal cortex is reduced in older adults

535   To investigate the sensitivity of brain regions to attention regulation in time, alpha-power time courses

536   were analyzed for the superior temporal and superior parietal cortical regions (Figure 8).

Figure 8: Alpha-power time courses for two anatomically defined regions of interest. A: Superior temporal cortex region. Alpha power time courses for both cue conditions (first half; second half) for both age groups, and time courses for the difference between cue conditions. Colored lines at the bottom indicate a significant difference from zero for the related time course (p ≤ 0.05, FDR-thresholded). The black line indicates a significant difference between time courses. Shadings around mean time courses reflect the standard error of the mean. **B:** Same as panel A for the superior parietal cortex region.

537   For younger people, alpha-power differences between cue conditions (first half; second half)

538   were strongest in superior parietal cortex, whereas no difference was observed for superior temporal

539   cortex (Figure 8). For older people, differences between cue conditions were present in both the

540   superior temporal and the superior parietal regions (Figure 8), consistent with the different source

541   configurations in older adults (Figure 6E/F).

Figure 9: Alpha power in the 0.8-s interval prior to the 2.5 s during which a gap could occur (first interval: 1–1.8 s; second interval: 5.5–6.3 s). The Cue × Time Interval interaction was greater in the superior parietal cortex for younger compared to older adults, whereas age groups did not differ for the superior temporal cortex (Cue × Time Interval × Region × Age Group interaction: p = 1.48 × 10⁻⁴; A and B). Panel C shows the interaction as an Attention Modulation Index (AMI). AMI was calculated as the difference between the first and the second interval when participants were cued to first half, plus the difference between the second and the first interval when participants were cued to second half. Larger values mean a stronger modulation of alpha power by the attentional cue. *p ≤ 0.05; n.s. – not significant; STC – superior temporal cortex; SPC – superior parietal cortex

To statistically quantify age-group differences in attentional modulation of alpha activity, we

conducted an rmANOVA with factors Cue (first half; second half), Time Interval (first interval: 1–1.8 s;

second interval: 5.5–6.3 s), Region (STC; SPC), and Age Group (younger; older). The Cue × Time Interval

× Region × Age Group interaction was significant ($F_{1,49}$ = 16.935, p = 1.48 × 10⁻⁴, n_p^2 = 0.257; Figure 9A

and B). In younger adults, the Cue × Time Interval interaction was significant only for SPC, but not for

STC (Cue × Time Interval × Region: $F_{1,24}$ = 18.029, p = 2.83 × 10⁻⁴, n_p^2 = 0.429), showing that alpha power

in SPC, but not in STC, decreased from the 1–1.8 s (first interval) to 5.5–6.3 s (second interval) when

participants were cued to the first half of the sound, and increased from the 1–1.8 s to 5.5–6.3 s intervals
when participants were cued to second half of the sound. In older adults, the Cue × Time Interval
interaction ($F_{1,25} = 9.885$, p = 0.004, $n_p^2 = 0.283$) was not further specified by brain region (Cue × Time
Interval × Region: $F_{1,25} = 2.466$, p = 0.129, $n_p^2 = 0.09$).

To examine the Cue × Time Interval × Region × Age Group interaction in a different way, we also
calculated an attentional modulation index (AMI) as the sum of the difference between time intervals
(i.e., difference between first and second interval for cued to first half, plus the difference between
second and first interval for cued to second half), separately for each participant and region. The
attentional modulation was larger in SPC for younger than older adults ($t_{49} = 2.094$, p = 0.041, d = 0.587),
whereas there was no difference between age groups for STC ($t_{49} = -0.829$, p = 0.411, d = 0.232; Region
× Age-Group interaction: $F_{1,49} = 16.935$, p = 1.48×10^{-4}, $n_p^2 = 0.257$; Figure 9C).

In sum, the source localization data indicate age-related differences in the brain regions
underlying listening-related alpha activity. Alpha power and alpha-power modulations by attention were
largest in superior parietal cortex in younger adults, whereas these effects were reduced in older adults.
In contrast, older adults exhibit an activation maximum located more ventro-laterally in the brain,
covering posterior temporal cortex. Below, we discuss how this age difference in the brain regions
underlying dynamic attention regulation may be the result of more proactive (younger) vs reactive
(older) cognitive control strategies during challenging listening.

General discussion

We investigated the neural processes involved when individuals listen attentively at specific points in
time and whether these processes differ between younger and older adults. We demonstrate that alpha
power indicates when in time individuals listen attentively (Experiment 1) and that alpha power is
modulated by listening difficulty, perhaps reflecting how much attention is deployed (Experiment 2).
Our data show that older adults are able to regulate attention in time, but that younger and older adults
recruit different brain regions during attentive listening. Younger adults show strongest attention-
related modulation of alpha power in superior parietal cortex, whereas older adults show strongest
modulations in posterior temporal cortex and reduced activity in superior parietal cortex (Experiment
3). We suggest that differences in source location between younger and older groups may be the result

of different cognitive control strategies employed to regulate attention in time during challenging

listening.

Alpha power is sensitive to critical aspects of dynamic attention regulation during listening

We demonstrate that neural alpha power in superior parietal cortex reflects individuals' directed

attention to points in time when key information is expected to occur during challenging listening

(Figures 2, 4, 6, and 8). Our work is consistent with studies showing that alpha power aligns temporally

with anticipated visual stimuli (Rohenkohl and Nobre, 2011; Bonnefond and Jensen, 2012; Payne et al.,

2013). Previous work also suggests that alpha activity is sensitive to temporally dynamic auditory

attention, where alpha power synchronizes with attended words presented during dichotic speech

listening (Wöstmann et al., 2016; Tune et al., 2018; Wöstmann et al., 2021). We show that alpha power

reflects expectations about when key auditory information will occur, thus indexing dynamic attention

deployment.

Alpha power has been shown to increase when individuals listen attentively to auditory stimuli

relative to a baseline, passive listening, or visual stimulation (Adrian, 1944; Foxe et al., 1998; Wöstmann

et al., 2015; Wöstmann et al., 2016; Dimitrijevic et al., 2017; Henry et al., 2017; Wöstmann et al., 2019;

Fiedler et al., 2021). Alpha power also increases in the hemisphere that is ipsilateral (relative to

contralateral) to the side to which a listener attends (Banerjee et al., 2011; Tune et al., 2018; Dahl et al.,

2019; Deng et al., 2020; Tune et al., 2021). Our data demonstrate that alpha power also indicates the

degree to which a listener deploys attention based on expected listening difficulty (Figure 4). Alpha

power was greater when participants expected gap detection to be difficult compared to easy, although

this was only observed when participants expected the gap to occur within ~4 s after sound onset.

Estimating the precise timing of temporally more distant events is more difficult (Gibbon, 1977;

Wearden, 2003; Buhusi and Meck, 2005; Grondin, 2014). Along these lines, we observed lower overall

performance (Figure 1 and 5) and a smaller hazard-rate effect (Figure 1) when participants attended to

the second compared to the first half of the sound. High levels of attention may thus have been needed

for the detection of gaps in the second half of the sound, independent of whether gap detection was

expected to be easy or difficult. This additional load may have led to the increase in alpha power for

both difficulty conditions when participants attended to the second half of the sound (Figure 4B/C). Our

results are compatible with the idea that dynamic attention enables enable listeners to budget mental

resources effectively, allocating enough resources moment to moment in order to achieve listening

goals.

Age differences in behavior may reflect different cognitive control strategies

The hazard-rate effect for response times indicates that both age groups oriented attention in time

(Figure 5; Nobre et al., 2007; Nobre and van Ede, 2018). Some previous studies have suggested older

adults may not use information to orient attention in time as well as younger adults do (Vallesi et al.,

2009; Zanto et al., 2011; Heideman et al., 2018), whereas this was not observed in other studies (Chauvin

et al., 2016; Droit-Volet et al., 2019). Interpretation of these results is difficult, however, because older

adults often responded overall more slowly than younger adults. Here, overall responses times were

similar between age groups. The comparable hazard-rate effect in both age groups suggests that older

adults are well able to orient attention in time during listening. Gap-detection performance, in contrast,

differed between age-groups. Younger individuals detected more gaps when they occurred later,

compared to earlier, within each cued sound half, whereas older individuals detected fewer (Figure 5).

The cognitive-control literature distinguishes between 'proactive' and 'reactive' control (Braver

et al., 2007; Braver, 2012). Proactive cognitive control is anticipatory and refers to the active and

sustained maintenance of goals and related information to facilitate task performance. In contrast,

reactive cognitive control is not anticipatory: goals and contextual information are only transiently

activated and decay faster (Braver et al., 2007). Behavioral performance in tasks requiring attentional

orienting will thus depend on the cognitive control strategy employed (Braver et al., 2007). Critically,

proactive control may be impaired in older adults, whereas reactive control has been suggested to

remain intact in older adulthood (Braver et al., 2007; Braver, 2012). In the current listening task,

decreasing hit rates for later gaps within a cued sound half for older adults may indicate a decay in

maintenance of goal and context information reflective of more reactive strategy.

Our data provide other indications that temporal information is somewhat less anticipatorily

utilized by older adults. Whereas response times depended on when a gap occurred in the first

compared to the second half of the sound in younger adults (Figures 1B and 5B), this difference was

clearly absent in older adults (Figure 5B). In fact, the influence of gap time on response times was very

similar for younger adults cued to the second sound half and those for older adults cued to either sound

half (Figure 5B, the decrease in response times with gap time for older adults' was also smaller compared

to the response-time decrease for younger adults cued to the first half; for all p < 0.05, one-sided). This

may suggest that older adults, while orienting attention in time, may have done so less effectively. We

speculate that the pattern of hit rates and responses times is consistent with older adults employing a

mixture of proactive and reactive cognitive control strategies, compared to younger adults, who relied

more on a proactive strategy.

Older adults recruit different brain regions for dynamic attention regulation than younger adults

Consistent with previous reports, we show an age-related reduction of alpha activity in superior parietal

cortex (Figure S2; Sander et al., 2012; Vaden et al., 2012; Deiber et al., 2013; Hong et al., 2015;

Wöstmann et al., 2015; Henry et al., 2017; Leenders et al., 2018; Rogers et al., 2018; Bonacci et al., 2019;

Getzmann et al., 2020), suggesting that parietal cortex is less involved in challenging attention tasks in

older adults.

Alpha power reflected attentional orienting in time for both younger and older adults (Figures 6,

8), but the recruited brain regions differed between age groups. Alpha activity in superior parietal cortex

was modulated by attention in younger adults (Tuladhar et al., 2007; van Dijk et al., 2008; Tune et al.,

2018), whereas older adults showed attention-related modulations in posterior temporal cortex (Figures

6, 8, 9). Previous studies using visuo-spatial attention tasks have reported reduced attention-related

lateralization of parietal alpha power for older compared to younger adults (Sander et al., 2012; Deiber

et al., 2013; Hong et al., 2015; Mok et al., 2016; Heideman et al., 2018; Leenders et al., 2018; Getzmann

et al., 2020). Source localization was not conducted in these previous studies, which may therefore have

missed brain regions sensitive to attention regulation in older adults. Other research in the auditory

domain shows the presence of alpha-power lateralization in a spatial-attention task in middle-aged to

older adults, but comparisons with younger individuals were not conducted (Tune et al., 2018; Tune et

al., 2021).

Proactive cognitive control is associated with sustained activity in prefrontal cortex (Braver et al.,

2007; Braver, 2012). Prefrontal cortex, in turn, is thought to orchestrate other task-relevant regions by

providing representation and maintenance of contextual information, such as the attention cue used

here (Braver et al., 2007). Parietal cortex is crucial for performance of tasks with attentional load

(Kanwisher and Wojciulik, 2000; Pessoa et al., 2003; Braver, 2012; Power and Petersen, 2013; Zanto and

Gazzaley, 2017) and may, in younger adults, reflect the outcome of cognitive control processes in

prefrontal cortex. Reactive control can involve other brain regions, such as anterior cingulate or other
more posterior cortices, including temporal cortex, to mediate performance in challenging tasks (Speer
et al., 2003; Braver et al., 2007; Dew et al., 2011; Braver, 2012). Recruitment of different brain regions
in older compared to younger adults in the current study could thus indicate more reliance on reactive
control processes.

Conclusions

We investigated the neural processes involved when individuals listen attentively at specific points in
time and whether these processes differ between younger and older adults. Alpha power reflected when
in time individuals listen attentively and was modulated by listening difficulty, indicating that alpha
reflects how much attention is deployed. Critically, our data show that older adults are able to regulate
attention in time during listening, but that they appear to use different behavioral listening strategies
and recruit different brain regions than do younger adults. Younger adults show attention-related
modulations of alpha power in superior parietal cortex, whereas older adults show attention-related
modulation in posterior temporal cortex. We suggest that the observed age-group differences in
recruited neural circuits and behavior reflect different cognitive control strategies employed to regulate
attention in time during challenging listening.

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Conflict of Interest

687   The authors have no conflict of interest.

Author Contributions

688   BH conceptualized and designed the study, recorded and analyzed the data, and wrote the manuscript.

690   BM assisted with MEG data acquisition and MEG data analysis, and edited the manuscript. MJH and JO

691   provided conceptual support and edited the manuscript. ISJ conceptualized and designed the study and

692   edited the manuscript.

References

Adrian ED (1944) Brain rhythms. Nature 153:360-362.

Banerjee S, Snyder AC, Molholm S, Foxe JJ (2011) Oscillatory Alpha-Band Mechanisms and the Deployment of Spatial Attention to Anticipated Auditory and Visual Target Locations: Supramodal or Sensory-Specific Control Mechanisms? The Journal of Neuroscience 31:9923-9932.

Başar E, Schürmann M, Başar-Eroglu C, Karakaş S (1997) Alpha oscillations in brain functioning: an integrative theory. International Journal of Psychophysiology 26:5-29.

Bell AJ, Sejnowski TJ (1995) An information maximization approach to blind separation and blind deconvolution. Neural Computation 7:1129-1159.

Berger H (1929) Über das Elektrenkephalogramm des Menschen. European Archives of Psychiatry and Clinical Neuroscience 87:527-570.

Besl PJ, McKay ND (1992) A method for registration of 3-D shapes. IEEE Transactions On Pattern Analysis And Machine Intelligence 14:239-256.

Billig AJ, Herrmann B, Rhone AE, Gander PE, Nourski KV, Snoad BF, Kovach CK, Kawasaki H, Howard III MA, Johnsrude IS (2019) A sound-sensitive source of alpha oscillations in human non-primary auditory cortex. The Journal of Neuroscience 39:8679-8689.

Bollimunta A, Cheng Y, Schroeder CE, Ding M (2008) Neuronal Mechanisms of Cortical Alpha Oscillations in Awake-Behaving Macaques. The Journal of Neuroscience 28:9976-9988.

Bonacci LM, Dai L, Shinn-Cunningham BG (2019) Weak neural signatures of spatial selective auditory attention in hearing-impaired listeners. The Journal of the Acoustical Society of America 146:2577-2589.

Bonnefond M, Jensen O (2012) Alpha Oscillations Serve to Protect Working Memory Maintenance against Anticipated Distracters. Current Biology 22:1969-1974.

Braver TS (2012) The variable nature of cognitive control: a dual mechanisms framework. Trends in Cognitive Sciences 16:106-113.

Braver TS, Barch DM (2002) A theory of cognitive control, aging cognition, and neuromodulation. Neuroscience and Biobehavioral Reviews 26:809-817.

Braver TS, Gray JR, Burgess GC (2007) Explaining the many varieties of working memory variation: Dual mechanisms of cognitive control. In: Variation in working memory (Conway A, Jarrold C, Kane M, Miyake A, Towse J, eds), pp 76-106. New York, NY, US: Oxford University Press.

Brehm JW, Self EA (1989) The Intensity of Motivation. Annual Review of Psychology 40:109-131.

Buhusi CV, Meck WH (2005) What makes us tick? Functional and neural mechanisms of interval timing. Nature Reviews Neuroscience 6:755-765.

Capilla A, Schoffelen J-M, Paterson G, Thut G, Gross J (2014) Dissociated α-Band Modulations in the Dorsal and Ventral Visual Pathways in Visuospatial Attention and Perception. Cerebral Cortex 24:550-561.

Chauvin JJ, Gillebert CR, Rohenkohl G, Humphreys GW, Nobre AC (2016) Temporal orienting of attention can be preserved in normal aging. Psychology and Aging 31:442-455.

Dahl MJ, Ilg L, Li S-C, Passow S, Werkle-Bergner M (2019) Diminished pre-stimulus alpha-lateralization suggests compromised self-initiated attentional control of auditory processing in old age. NeuroImage 197:414-424.

Deiber M-P, Ibañez V, Missonnier P, Rodriguez C, Giannakopoulos P (2013) Age-associated modulations of cerebral oscillatory patterns related to attention control. NeuroImage 82:531-546.

Deng Y, Choi I, Shinn-Cunningham B (2020) Topographic specificity of alpha power during auditory spatial attention. NeuroImage 207:116360.

Dew ITZ, Buchler N, Dobbins IG, Cabeza R (2011) Where Is ELSA? The Early to Late Shift in Aging. Cerebral Cortex 22:2542-2553.

Dimitrijevic A, Smith ML, Kadis DS, Moore DR (2017) Cortical Alpha Oscillations Predict Speech Intelligibility. Frontiers in Human Neuroscience 11:Article 88.

Droit-Volet S, Lorandia F, Coull JT (2019) Explicit and implicit timing in aging. Acta Psychologica 193:180-189.

Fiedler L, Ala TS, Graversen C, Alickovic E, Lunner T, Wendt D (2021) Hearing Aid Noise Reduction Lowers the Sustained Listening Effort During Continuous Speech in Noise—A Combined Pupillometry and EEG Study. Ear & Hearing 42:1590-1601.

Fischl B, Sereno MI, Dale AM (1999a) Cortical surface-based analysis II: inflation, flattening, and a surface-based coordinate system. NeuroImage 9:195-207.

Fischl B, Sereno MI, Tootell RBH, Dale AM (1999b) High-resolution intersubject averaging and a coordinate system for the cortical surface. Human Brain Mapping 8:272-284.

Fitzgibbons PJ, Gordon-Salant S (2010) Behavioral Studies With Aging Humans: Hearing Sensitivity and Psychoacoustics. In: The Aging Auditory System (Gordon-Salant S, Frisina RD, Popper AN, Fay RR, eds), pp 111-134. New York, USA: Springer-Verlag.

Foxe JJ, Simpson GV, Ahlfors SP (1998) Parieto-occipital ~10Hz activity reflects anticipatory state of visual attention mechanisms. NeuroReport 9:3929-3933.

Fu K-MG, Foxe JJ, Murray MM, Higgins BA, Javitt DC, Schroeder CE (2001) Attention-dependent suppression of distracter visual input can be cross-modally cued as indexed by anticipatory parieto–occipital alpha-band oscillations. Cognitive Brain Research 12:145-152.

Garcés P, López-Sanz D, Maestú F, Pereda E (2017) Choice of Magnetometers and Gradiometers after Signal Space Separation. Sensors 17:2926.

Gatehouse S, Noble W (2004) The speech, spatial and qualities of hearing scale (SSQ). International Journal of Audiology 43:85-99.

Getzmann S, Klatt L-I, Schneider D, Begau A, Wascher E (2020) EEG correlates of spatial shifts of attention in a dynamic multi-talker speech perception scenario in younger and older adults. Hearing Research 398:108077.

Gibbon J (1977) Scalar expectancy theory and Weber's law in animal timing. Psychological Review 84:279-325.

Glasser MF, Coalson TS, Robinson EC, Hacker CD, Harwell J, Yacoub E, Ugurbil K, Andersson J, Beckmann CF, Jenkinson M, Smith SM, Van Essen DC (2016) A multi-modal parcellation of human cerebral cortex. Nature 536:171-178.

Grondin S (2014) About the (non)scalar property for time perception. Advances in experimental medicine and biology 829:17-32.

Gross J, Kujala J, Hämäläinen MS, Timmermann L, Schnitzler A, Salmelin R (2001) Dynamic imaging of coherent sources: Studying neural interactions in the human brain. Proceedings of the National Academy of Sciences 98:694-699.

Hämäläinen MS, Hari R (2002) Magnetoencephalographic (MEG) Characterization of Dynamic Brain Activation: Basic Principles and Methods of Data Collection and Source Analysis. In: Brain Mapping: The Methods (Toga AW, Mazziotta JC, eds), pp 227-253: Academic Press.

Hämäläinen MS, Hari R, Ilmoniemi RJ, Knuutila J, Lounasmaa OV (1993) Magnetoencephalography – theory, instrumentation, and applications to noninvasive studies of the working human brain. Reviews of Modern Physics 65:413-497.

Han X, Jovicich J, Salat DH, van der Kouwe A, Quinn B, Czanner S, Busa E, Pacheco J, Albert M, Killiany R, Maguire P, Rosas D, Makris N, Dale AM, Dickerson B, Fischl BR (2006) Reliability of MRI-derived measurements of human cerebral cortical thickness: The effects of field strength, scanner upgrade and manufacturer. NeuroImage 32:180-194.

Heideman SG, Rohenkohl G, Chauvin JJ, Palmer CE, van Ede F, Nobre AC (2018) Anticipatory neural dynamics of spatial-temporal orienting of attention in younger and older adults. NeuroImage 178:46-56.

Henry MJ, Obleser J (2012) Frequency modulation entrains slow neural oscillations and optimizes human listening behavior. Proceedings of the National Academy of Sciences 109:20095-20100.

Henry MJ, Herrmann B, Obleser J (2014) Entrained neural oscillations in multiple frequency bands co-modulate behavior. Proceedings of the National Academy of Sciences 111:14935-14940.

Henry MJ, Herrmann B, Obleser J (2016) Neural microstates govern perception of auditory input without rhythmic structure. The Journal of Neuroscience 36:860-871.

Henry MJ, Herrmann B, Kunke D, Obleser J (2017) Aging affects the balance of neural entrainment and top-down neural modulation in the listening brain. Nature Communications 8:15801.

Herrmann B, Johnsrude IS (2018) Attentional State Modulates the Effect of an Irrelevant Stimulus Dimension on Perception. Journal of Experimental Psychology: Human Perception and Performance 44:89-105.

Herrmann B, Johnsrude IS (2020) A Model of Listening Engagement (MoLE). Hearing Research.

Herrmann B, Maess B, Johnsrude IS (2018) Aging Affects Adaptation to Sound-Level Statistics in Human Auditory Cortex. The Journal of Neuroscience 38:1989-1999.

Hong X, Sun J, Bengson JJ, Mangun GR, Tong S (2015) Normal aging selectively diminishes alpha lateralization in visual spatial attention. NeuroImage 106:353-363.

Hornsby BW, Naylor G, Bess FH (2016) A Taxonomy of Fatigue Concepts and Their Relation to Hearing Loss. Ear & Hearing 37:136S-144S.

Humes LE, Busey TA, Craig JC, Kewley-Port D (2009) The effects of age on sensory thresholds and temporal gap detection in hearing, vision, and touch. Attention, Perception, & Psychophysics 71:860-871.

Jensen O, Mazaheri A (2010) Shaping functional architecture by oscillatory alpha activity: gating by inhibition. Frontiers in Human Neuroscience 4:Article 186.

Johnsrude IS, Rodd JM (2016) Factors That Increase Processing Demands When Listening to Speech. In: Neurobiology of Language (Hickok G, Small SL, eds), pp 491-502: Elsevier Academic Press.

Kanwisher N, Wojciulik E (2000) Visual attention: Insights from brain imaging. Nature Reviews
Neuroscience 1:91-100.
Klimesch W (1999) EEG alpha and theta oscillations reflect cognitive and memory performance: a
review and analysis. Brain Research Reviews 29:169-195.
Klimesch W, Sauseng P, Hanslmayr S (2007) EEG alpha oscillations: The inhibition–timing hypothesis.
Brain Research Reviews 53:63-88.
Leenders MP, Lozano-Soldevilla D, Roberts MJ, Jensen O, De Weerd P (2018) Diminished Alpha
Lateralization During Working Memory but Not During Attentional Cueing in Older Adults.
Cerebral Cortex 28:21-32.
Lehtelä L, Salmelin R, Hari R (1997) Evidence for reactive magnetic 10-Hz rhythm in the human
auditory cortex. Neuroscience Letters 222:111-114.
Makeig S, Bell AJ, Jung T-P, Sejnowski TJ (1996) Independent component analysis of
electroencephalographic data. In: Advances in Neural Information Processing Systems
(Touretzky D, Mozer M, Hasselmo M, eds). Cambridge, MA, USA: MIT Press.
Mattys SL, Davis MH, Bradlow AR, Scott SK (2012) Speech recognition in adverse conditions: A
review. Language and Cognitive Processes 27:953-978.
Mok RM, Myers NE, Wallis G, Nobre AC (2016) Behavioral and Neural Markers of Flexible Attention
over Working Memory in Aging. Cerebral Cortex 26:1831-1842.
Müller N, Leske S, Hartmann T, Szebényi S, Weisz N (2015) Listen to yourself: The medial prefrontal
cortex modulates auditory alpha power during speech preparation. Cerebral Cortex 25:4029-
4037.
Niedermeyer E (1990) Alpha-like rhythmical activity of the temporal lobe. Clinical
Electrocencephalography 21:210-224.
Niemi P, Näätänen R (1981) Foreperiod and simple reaction time. Psychological Bulletin 89:133-162.
Nobre AC, van Ede F (2018) Anticipated moments: temporal structure in attention. Nature Reviews
Neuroscience 19:34-48.
Nobre AC, Correa A, Coull JT (2007) The hazards of time. Current Opinion in Neurobiology 17:465-
470.
Nolte G (2003) The magnetic lead field theorem in the quasi-static approximation and its use for
magnetoencephalography forward calculation in realistic volume conductors. Physics in
Medicine and Biology 48:3637–3652.
Obleser J, Wöstmann M, Hellbernd N, Wilsch A, Maess B (2012) Adverse Listening Conditions and
Memory Load Drive a Common Alpha Oscillatory Network. The Journal of Neuroscience
32:12376-12383.
Oostenveld R, Fries P, Maris E, Schoffelen JM (2011) FieldTrip: Open source software for advanced
analysis of MEG, EEG, and invasive electrophysiological data. Computational Intelligence and
Neuroscience 2011:Article ID 156869.
Palva S, Palva JM (2011) Functional roles of alpha-band phase synchronization in local and large-scale
cortical networks. Frontiers in Psychology 2:Article 204.
Payne L, Guillory S, Sekuler R (2013) Attention-modulated Alpha-band Oscillations Protect against
Intrusion of Irrelevant Information. Journal of Cognitive Neuroscience 25:1463-1476.
Peelle JE (2018) Listening Effort: How the Cognitive Consequences of Acoustic Challenge Are
Reflected in Brain and Behavior. Ear & Hearing 39:204-214.
Pessoa L, Kastner S, Ungerleider LG (2003) Neuroimaging Studies of Attention: From Modulation of
Sensory Processing to Top-Down Control. The Journal of Neuroscience 23:3990-3998.

Pichora-Fuller MK (2003) Processing speed and timing in aging adults: psychoacoustics, speech perception, and comprehension. International Journal of Audiology 42:S59-S67.

Pichora-Fuller MK (2016) How Social Psychological Factors May Modulate Auditory and Cognitive Functioning During Listening. Ear & Hearing 37 Suppl 1:92S-100S.

Pichora-Fuller MK, Kramer SE, Eckert MA, Edwards B, Hornsby BWY, Humes LE, Lemke U, Lunner T, Matthen M, Mackersie CL, Naylor G, Phillips NA, Richter M, Rudner M, Sommers MS, Tremblay KL, Wingfield A (2016) Hearing Impairment and Cognitive Energy: The Framework for Understanding Effortful Listening (FUEL). Ear & Hearing 37 Suppl 1:5S-27S.

Power JD, Petersen SE (2013) Control-related systems in the human brain. Current Opinion in Neurobiology 23:223-228.

Richter M, Gendolla GHE, Wright RA (2016) Three Decades of Research on Motivational Intensity Theory: What We Have Learned About Effort and What We Still Don't Know. In: Advances in Motivation Science (Elliot AJ, ed), pp 149-186. Cambridge, MA, USA: Academic Press.

Rogers CS, Payne L, Maharjan S, Wingfield A, Sekuler R (2018) Older Adults Show Impaired Modulation of Attentional Alpha Oscillations: Evidence From Dichotic Listening. Psychology and Aging 33:246-258.

Rohenkohl G, Nobre AC (2011) Alpha Oscillations Related to Anticipatory Attention Follow Temporal Expectations. The Journal of Neuroscience 31:14076-14084.

Sander MC, Werkle-Bergner M, Lindenberger U (2012) Amplitude modulations and inter-trial phase stability of alpha-oscillations differentially reflect working memory constraints across the lifespan. NeuroImage 59:646-654.

Shenhav A, Musslick S, Lieder F, Kool W, Griffiths TL, Cohen JD, Botvinick MM (2017) Toward a Rational and Mechanistic Account of Mental Effort. Annual Review of Neuroscience 40:99-124.

Snell KB (1997) Age-related changes in temporal gap detection. The Journal of the Acoustical Society of America 101:2214-2220.

Speer NK, Jacoby LL, Braver TS (2003) Strategy-dependent changes in memory: Effects on behavior and brain activity. Cognitive, Affective, & Behavioral Neuroscience 3:155-167.

Strauss DJ, Francis AL (2017) Toward a taxonomic model of attention in effortful listening. Cognitive, Affective & Behavioral Neuroscience 17:809-825.

Strouse A, Ashmead DH, Ohde RN, Grantham DW (1998) Temporal processing in the aging auditory system. The Journal of the Acoustical Society of America 104:2385-2399.

Taulu S, Kajola M, Simola J (2004) Suppression of Interference and Artifacts by the Signal Space Separation Method. Brain Topography 16:269-275.

Taulu S, Simola J, Kajola M (2005) Applications of the Signal Space Separation Method. IEEE Transactions On Signal Processing 53:3359-3372.

Tiihonen J, Hari R, Kajola M, Karhu J, Ahlfors SP, Tissari S (1991) Magnetoencephalographic 10-Hz rhythm from the human auditory cortex. Neuroscience Letters 129:303-305.

Tuladhar AM, Huurne Nt, Schoffelen J-M, Maris E, Oostenveld R, Jensen O (2007) Parieto-Occipital Sources Account for the Increase in Alpha Activity with Working Memory Load. Human Brain Mapping 28:785-792.

Tune S, Wöstmann M, Obleser J (2018) Probing the limits of alpha power lateralisation as a neural marker of selective attention in middle-aged and older listeners. European Journal of Neuroscience 48:2537-2550.

Tune S, Alavash M, Fiedler L, Obleser J (2021) Neural attentional-filter mechanisms of listening success in middle-aged and older individuals. Nature Communications 12:4533.

Vaden RJ, Hutcheson NL, McCollum LA, Kentros J, Visscher KM (2012) Older adults, unlike younger adults, do not modulate alpha power to suppress irrelevant information. NeuroImage 63:1127-1133.

Vallesi A, McIntosh AR, Stuss DT (2009) Temporal preparation in aging: A functional MRI study. Neuropsychologia 47:2876-2881.

van Dijk H, Schoffelen J-M, Oostenveld R, Jensen O (2008) Prestimulus Oscillatory Activity in the Alpha Band Predicts Visual Discrimination Ability. The Journal of Neuroscience 28:1816-1823.

Wearden JH (2003) Applying the scalar timing model to human time psychology: Progress and challenges. In: Time and mind II: Information processing perspectives., pp 21-39. Ashland, OH, US: Hogrefe & Huber Publishers.

Westbrook A, Braver TS (2015) Cognitive effort: A neuroeconomic approach. Cognitive, Affective & Behavioral Neuroscience 15:395-415.

Wilsch A, Henry MJ, Herrmann B, Maess B, Obleser J (2015) Alpha Oscillatory Dynamics Index Temporal Expectation Benefits in Working Memory. Cerebral Cortex 25:1938-1946.

Wöstmann M, Alavash M, Obleser J (2019) Alpha Oscillations in the Human Brain Implement Distractor Suppression Independent of Target Selection. The Journal of Neuroscience 39:9797-9805.

Wöstmann M, Schmitt L-M, Obleser J (2020) Does Closing the Eyes Enhance Auditory Attention? Eye Closure Increases Attentional Alpha-Power Modulation but Not Listening Performance. Journal of Cognitive Neuroscience 32:212-225.

Wöstmann M, Maess B, Obleser J (2021) Orienting auditory attention in time: Lateralized alpha power reflects spatio-temporal filtering. NeuroImage 228:117711.

Wöstmann M, Herrmann B, Wilsch A, Obleser J (2015) Neural Alpha Dynamics in Younger and Older Listeners Reflect Acoustic Challenges and Predictive Benefits. The Journal of Neuroscience 35:1458-1467.

Wöstmann M, Herrmann B, Maess B, Obleser J (2016) Spatiotemporal dynamics of auditory attention synchronize with speech. Proceedings of the National Academy of Sciences 113:3873-3878.

Zanto TP, Gazzaley A (2017) Cognitive Control and the Ageing Brain. In: The Wiley Handbook of Cognitive Control (Egner T, ed), pp 476-490: John Wiley & Sons.

Zanto TP, Pan P, Liu H, Bollinger J, Nobre AC, Gazzaley A (2011) Age-related changes in orienting attention in time. The Journal of Neuroscience 31:12461-12470.