Cortical patterns shift from sequence feature separation during planning to integration during motor execution

Rhys Yewbrey[1,2], Myrto Mantziara[1], Katja Kornysheva[1,2]*

[1] Bangor Imaging Unit, Bangor University, Bangor, Wales LL57 2AS, UK

[2] Centre for Human Brain Health, School of Psychology, University of Birmingham, Birmingham, B15 2TT, UK

*Correspondence: Dr Katja Kornysheva at k.kornysheva@bham.ac.uk, Centre for Human Brain Health, School of Psychology, University of Birmingham, Birmingham, B15 2TT, UK

Word count: Abstract: 241; Introduction: 631; Results: 2090; Discussion: 1376; Materials and Methods: 3034; 27 pages, 5 main Figures; 2 Supplementary Figures; 2 Supplementary Tables.

Author contributions: R.Y., M.M. and K.K. conceived the experiments; R.Y., and K.K. formulated the hypotheses; R.Y., M.M. and K.K. collected the data; R.Y. and K.K. designed the analysis; R.Y. and K.K. performed the analyses; R.Y. and K.K. wrote the original version of the manuscript; All authors contributed to editing of the manuscript.

Acknowledgements: The authors wish to thank David McKiernan for the construction and technical support of the force keyboard device, and Prof Paul Downing, Prof Paul Mullins, and Dr Ken Valyear for their useful comments on the study design and MRI acquisition. This work was supported by the Academy of Medical Sciences Springboard Award (SBF006\1052, K.K.).

Disclosures: The authors declare no conflicts of interest.

ABSTRACT

Performing sequences of movements from memory and adapting them to changing task
demands is a hallmark of skilled human behaviour, from handwriting to playing a musical
instrument. Prior studies showed a fine-grained tuning of cortical primary motor, premotor,
and parietal regions to motor sequences – from the low-level specification of individual
movements to high-level sequence features like sequence order and timing. However, it is
not known how tuning in these regions unfolds dynamically across planning and execution.
To address this, we trained 24 healthy right-handed participants to produce four five-
element finger press sequences with a particular finger order and timing structure in a
delayed sequence production paradigm entirely from memory. Local cortical fMRI patterns
during preparation and production phases were extracted from separate 'No-Go' and 'Go'
trials, respectively, to tease out activity related to these peri-movement phases. During
sequence planning, premotor and parietal areas increased tuning to movement order and
timing, irrespective of their combinations. In contrast, patterns reflecting the unique
integration of sequence features emerged in these regions during execution only, alongside
timing-specific tuning in the ventral premotor, supplementary motor, and superior parietal
areas. This was in line with the participants' behavioural transfer of trained timing, but not
of order to new sequence feature combinations. Our findings suggest a general neural state
shift from high-level feature separation to low-level feature integration within cortical
regions for movement execution. Recompiling sequence features trial-by-trial during
planning may enable flexible last-minute adjustment before movement initiation.

INTRODUCTION

Skilled sequences of movements performed from memory are regarded as a hallmark of
human dexterity [1–3]. They are essential building blocks of everyday skilled behaviours, from
typing and handwriting, to tying shoelaces, or playing a musical instrument (Figure 1a). In
addition to the order of movements in a sequence, the temporal accuracy of the
movements can be crucial to the success of the task, such as when typing a Morse code, or
performing a martial arts sequence. While our knowledge of the neural control of motor
sequences in the primate brain, particularly across cortical regions, has significantly
expanded over the last decade, it is not well understood how higher-order features of
sequences such as movement order and timing are integrated trial-by-trial for skilled
performance.

Previous behavioural [4–6], computational [7,8], neurophysiological [9–11] and neuroimaging
findings [12–14] have established that movement order is controlled independently of timing,
and vice versa, whenever motor sequences incorporated temporally discrete sub-goals. This
includes sequences that are extensively trained and performed from memory without
external guidance, characteristic of motor sequence execution in the real world. The
integration of movement timing and order has been studied in the context of execution
[6,12,15–17], but we currently do not know whether movement order and timing integration
takes place prior to movement onset, and which brain regions hold this information about
the upcoming sequence.

Neural and haemodynamic activity patterns in contralateral primary motor and
sensorimotor, premotor, and parietal cortices show informational tuning to trained motor
sequences [12,18–25]. Specifically, activity patterns in motor-related regions outside the primary
motor cortex - the bilateral premotor, supplementary motor and parietal areas - contain
high-level information, e.g., about sequence chunks and positional rank in the sequence
[18,26,27] and spatial, rather than body-centred coordinates [22]. Further, activity patterns in
these regions can generalise across different pairings of movement order and timing [12]
(Figure 1b). In contrast, activity patterns in contralateral primary motor (M1) and
sensorimotor (S1) cortices contralateral to the movements are associated with the planning
and execution of single movements in a sequence [11,20,21,28] and are largely effector-specific
[22]. Further, activity in M1 has been shown to hold information about unique sequence order
and timing combinations, suggesting a lower-level integrated representation of the
sequences [12] (Figure 1b), but may also be reflecting patterns that are driven by differences
in the identity of the first movement in a sequence [20,26].

Despite the progress made, we lack knowledge of when and where motor-related cortical
areas integrate the order of movements with their timing for successful sequence
production. One possibility is that these regions show a fixed mapping to high-level
independent (premotor, parietal) or lower-level integrated (primary motor and
sensorimotor) features of sequences, respectively [12]. These may be activated simultaneously
or sequentially depending on the peri-movement phase, but their informational content
would remain stable (Figure 1c, "Fixed mapping"). Alternatively, the tuning of these regions
to high and low-level features of sequences may change dynamically depending on trial
phase, such that the same regions parse sequence order and timing during planning but
integrate these sequence features during execution (Figure 1c, "Dynamic mapping").

Here, we trained participants to produce five-element finger press sequences comprised
of two finger orders and two temporal interval orders (timings) from memory in a delayed
production paradigm. To disentangle planning from execution using fMRI, activity was
extracted from 'No-Go' and 'Go' trials, respectively. We utilised multivariate pattern analysis
to distinguish between independent (transferrable) and integrated (unique) BOLD patterns
related to the planned and executed sequence order and timing. Our results provide strong
evidence for the integration of sequence order and timing during sequence execution only,
but not during planning. Further, they support the idea that contralateral premotor to
parietal regions are not fixed in their informational content but update their tuning
dynamically.

Figure 1. Theoretical framework and hypotheses. (a) Skilled sequence production, e.g. when playing a
melody on a piano, is characterised by producing movements with a specific order and timing and combining
them flexibly trial-by-trial. (b) Previous findings localised independent patterns of order and timing to
premotor, supplementary motor, and parietal regions, while their integration was found in the primary motor
cortex (M1) [12]. (c) How does this mapping evolve across planning and execution? "Fixed mapping" hypotheses
state that premotor and parietal regions outside of M1 control order and timing as independent motor
sequence features, and M1 itself controls the non-linear integration of the two during planning and/or
production. In contrast, the "Dynamic mapping" hypothesis states that there is a state shift within regions
from independent feature control during planning to integration during execution (OSF preregistration:
https://doi.org/10.17605/OSF.IO/G64HV).

RESULTS

Discrete sequence production from memory

Participants were trained to produce four finger-press sequences from memory with the
right hand on a force transducer keyboard (Figure 2a). Training consisted of a three-staged
transition across two days from trials which visually guided sequence production, towards
trials which required sequence production entirely from memory (Figure 2b). During

functional MRI scans taking place on the third day, participants were required to produce
movement sequences from memory only (see supplementary table S1 for trial distribution).
Sequences were cued 1000-2500ms before the Go cue by a Sequence cue (abstract fractal
image) to prompt the planning of the respective sequence without movement (Figure 2c).
To isolate fMRI responses to movement planning without contamination from execution
patterns, in addition to 'Go' trials, 'No-Go' trials were implemented which consisted only of
the Sequence cue but did not contain a Go cue (Figure 2d). 'No-Go' trials made up 20% of
trials during training, and 50% of trials during the fMRI session (see Methods). The target
sequences were unique combinations of two finger orders consisting of five presses
matched in finger press occurrence and two target relative inter-press-interval (IPI) orders
involving four IPIs matched in target duration (Figure 2e). The finger orders were generated
pseudo-randomly for each participant, but each sequence started with the same finger
press within each participant to avoid first-finger identity driving the sequence decoding
during the preparatory period [20]. Timing 1 and Timing 2 were the same across participants.

The keyboard recorded isometric force trajectories from fingers of both the active right
and the passive left hand concurrently during preparation and production (Figure 2f, Figure
2g). Points were awarded trial-by-trial only if participants did not exceed a force threshold
above the baseline period during preparation and 'No-Go' trials. In 'Go' trials points were
calculated based on initiation time after the Go cue, finger press accuracy, and timing
accuracy. 'No-Go' trials were rewarded when no responses were made above threshold (see
Methods). To ensure that participants were not pre-pressing the keys below the force
threshold, we checked offline if exerted force of the right hand increased significantly above
the baseline level. In 'No-Go' trials we checked for force increase from the Sequence cue
onset to the last possible moment a Go cue could appear if it were a 'Go' trial, to represent
the preparatory period. Participants did not increase force during 'No-Go' trials, and instead
showed a small but significant force reduction (M = 0.154N, SD = 0.09) relative to baseline
(M = 0.162 N, SD = 0.09; $t(23)$ = 3.35, p = .003). A similar small decrease, rather than an
increase, was found in the preparation phase of 'Go' trials (M = 0.163 N, SD = 0.09) relative
to baseline (M = 0.164 N, SD = 0.09; $t(23)$ = 2.44, p = .023), suggesting that this force
decrease associated with planning was not specific to 'No Go' trials. Importantly the data
shows that participants did not engage in any subthreshold pre-pressing or rehearsal of the
sequence during sequence preparation.

Figure 2. Experimental and trial designs. (a) Participants produced finger presses on a ten-finger force transducer keyboard. The hands were visually occluded from the participants' view by a panel during training and when lying in a supine position during the fMRI session. Target fingers on the right hand are indicated by different colours that also correspond to the legend in later panels. Fingers on the left (inactive) hand are marked as black. (b) Trial type proportions on each experimental day progressed from 100% instructed

(Training 1) to 50/50% mixed (Training 2) to 100% from memory (Training 3) trials during the last stage of
training and during fMRI. Black hands with a grey background and a red finger cue indicate visually instructed
trials. Black hands with a green background represent trials with sequence production from memory. (c) 'Go'
trials from memory consisted of a Sequence cue, followed by a fixation cross and a Go cue instructing a
production period. The occurrence of the Go cue was the onset of the respective hand stimulus. The trial
ended with a feedback screen which indicated finger and temporal accuracy relative to a target sequence.
Instructed trials, shown as an insert at the top of the image, followed the same trial structure as from memory
trials, but displayed visual finger cues to aid production. (d) 'No-Go' trials consisted of a Sequence cue,
followed by a fixation cross without a Go cue, and feedback screen. (e) A raster plot shows all button press
timings in correct trials produced from memory across the entire fMRI session in one representative
participant. Horizontal lines separate the different sequences that followed a two finger order by two timing
design (see Methods for details). Vertical dotted lines indicate target press timings. Each coloured dot
represents a different effector, see corresponding legend. (f) Example force traces from 10 channels
corresponding to the fingers on the right (coloured) and left hands (black) in one representative 'Go' trial
during fMRI. The horizontal dashed line represents the finger press threshold, and coloured vertical lines
represent the time point at which a press was detected from the respective finger. (g) Example force traces, as
in f, from one representative 'No-Go' trial.

All included participants reached the criteria of producing different timing structures
(Timing 1 and 2) across finger orders (Order 1 and 2; Figure 3a shows group-level data,
ANOVA results in Methods). We did not expect any main effect or interactions with finger
order to be significant at the group level, due to the randomisation of trained finger orders
across participants (see Methods). However, we assessed the main effects of order and
timing, and their interaction at the individual level. Here 18 out of the 24 participants
showed a significant order by interval position interaction, and 10 showed a significant
three-way interaction between timing, order, and interval position. The presence of these
idiosyncratic press timing patterns at the individual level suggests the integration of
sequence order and timing features. Crucially, sequence timing error showed no difference
between timing structures suggesting that there were no systematic differences in difficulty
for Timing 1 and Timing 2 at the group level ($F(1,23) = 0.07$, $p = .792$, $\eta p^2 = .003$; Figure 3b).
At the individual level, 10 participants showed a significant main effect of order, 15 showed
a significant main effect of timing, and four showed a significant interaction between order
and timing, again suggesting an integration of the two sequence features.

To test for independent transfer of finger order and timing to new combinations before
and after training, participants performed a synchronisation task where we assessed their
synchronization error (absolute deviation from target timing) to a visually cued sequence
[14].The trials in each condition were presented in a blocked manner with 8 repetitions to
assess short-term learning gains related to trained finger order and timing (Figure 3c). Since
the transfer of trained sequence timing to a new finger order only takes place after three
exposures, synchronisation performance was only assessed from the fourth sequence
exposure onwards consistent with previously reported analyses [6,12,14]. During the post-
training phase, we compared each condition (trained, order transfer, timing transfer) to
completely new sequences ($M = 196.15ms$, $SD = 34.00$) in a one-tailed paired sample t-test,
with trained sequences ($M = 160.43ms$, $SD = 33.09$) showing a significant performance
advantage, as predicted ($t(23) = 6.34$, $p > .001$), as did timing transfer sequences ($M =$
182.10, $SD = 39.72$; $t(23) = 2.09$, $p = .024$), replicating previous findings [6,12,14] (Figure 3d). In
contrast to earlier reports, order transfer sequences ($M = 223.87$, $SD = 48.30$) showed a
significantly worse performance ($t(23) = 3.52$, $p = .002$, two-tailed test). Whilst knowledge of
both features of a sequence combined, or just its timing, facilitated task performance,
knowledge of sequence order hindered future learning of novel sequence acquisition when

paired with a new timing structure. This implies that the current participants acquired a
stronger independent representation of timing than of finger order which was integrated
with a particular timing structure during production.

Figure 3. Sequence timing and feature transfer. (a) Inter-press-interval (IPI) structure of the four trained
sequences during the fMRI session (day 3). A significant interaction between sequence timing and interval
position shows distinct IPI sequences between Timing 1 and Timing 2 across finger order sequences Order 1
and 2. (b) Timing error (normalised to the target interval durations, see Methods) during the fMRI session did
not differ between sequences. (c) Behavioural transfer results from the synchronisation task obtained from
instructed 'Go' cue trials following the last training stage on day 2. Absolute deviation from target timing are
shown across sequence repetitions for trained sequences (green), sequences with trained finger orders, but
unfamiliar timing (blue), sequences with trained timing, but unfamiliar order (red), and new sequences with
both unfamiliar finger order and timing (black). (d) Absolute deviation from target timing, as in a, extracted
from the fourth to the last sequence repetition as in previous work (e.g., Kornysheva et al. 2019). Significance
of t-tests to identify performance benefits compared to new sequences is shown by coloured asterisks and
horizontal lines. Note that the trained order condition showed a significant increase in synchronisation error (p
= .002, two-tailed t-test), suggesting interference rather than benefits related to sequence feature transfer. **
$p < 0.01$; * $p < 0.05$, one-sided t-test.

Activity increases during preparation and production

Percent signal change of preparation and production relative to rest were calculated to
identify areas with increased activity during these two respective phases of the task. While
preparatory activity was modelled in the GLM for both 'Go' and 'No-Go' trials, preparatory
activity for % signal change and multivariate pattern analyses was solely sampled from No-
Go trials to disentangle the BOLD activity in these two phases whilst keeping a fast event-
related design. We then calculated the percent signal change across the cortex (Figure 4a)
and extracted values along two cross-sections of the cortical surface on the contralateral
(left) side to the motor effector [12] (Figure 4b). These cross-sections extended from anterior
to posterior and ventral to dorsal, across premotor to parietal and premotor to
supplementary motor regions respectively, because our hypotheses (osf.io/g64hv) on the
imaging results during sequence preparation and production were put forward for
contralateral premotor, primary motor, and parietal regions, which we expected to be
tuned to sequence information based on previous studies [12,18–25]. Whole-brain results are
presented in the Supplementary Materials. We carried out one-tailed non-parametric
permutation tests along these cross-sections to identify significant clusters where activity
increased above baseline [29]. During preparation, a very small, but significant, activity
increase was found within ventral premotor cortex (PMv) (p = .002), and a marginally
significant increase found within dorsal premotor cortex (PMd) (p = .050) (Figure 4b). During
production, significant activity increases were found across the majority of contralateral
motor-related regions, with one large cluster across PMd, M1, sensorimotor cortex (S1),
anterior superior parietal cortex (SPCa), and posterior superior parietal cortex (SPCp) (p <
.001), and another cluster which spanned the cross-section from PMv to PMd (p < .001). The
cross-section overlapping with anterior supplementary motor area (SMA) did not show a
significant activity increase from rest during production. However, note that the section of
the SMA directly posterior to the cross-section did show a significant activity increase (see
supplementary Figure S1a and Table S2 for whole-brain contrast cluster analysis).

Figure 4. Percent signal change during preparation and production. (a) Inflated surface maps are shown in upper panels and flat maps in lower panels, displaying mean % signal change during preparation (left panels) and production relative to rest (right panels), respectively. (b) Mean % signal change relative to rest for both preparation (blue lines) and production (orange lines), plotted on cross-sections running from rostral premotor cortex, through the hand area, to the occipito-parietal junction (upper panel) and on a profile running from the ventral, through the dorsal premotor cortex, to the SMA (BA6; lower panel). Clusters with significant increases above baseline are denoted by the coloured horizontal lines and asterisks, calculated using one-tailed non-parametric permutation tests. Cing, cingulate; CS, central sulcus; IPS, intraparietal sulcus; m, medial wall; M1, primary motor cortex; OPJ, occipito-parietal junction; PMd, dorsal premotor cortex; PMv, ventral premotor

265   cortex; PoCS, post-central sulcus; PreCS, pre-central sulcus; pre-SMA, pre-supplementary motor area; S1,
266   sensorimotor cortex; SFS, superior frontal sulcus; SMA, supplementary motor area; SPCa, anterior superior
267   parietal cortex; SPCp, posterior superior parietal cortex. ** $p < 0.01$; * $p < 0.05$, one-sided t-test.

Multi-variate pattern analysis (MVPA)

We used MVPA to identify cortical areas that showed systematic changes in BOLD activity
patterns between sequences during preparation and production. Using a whole brain
searchlight of 160 voxels [30], we trained a linear discriminant analysis (LDA) classifier to
distinguish between sequences in a one-run-out cross-validation method – an approach that
has been validated with pattern simulations in a previous study [12]. Specifically, we looked
for regional activity patterns that either transferred across or were unique for specific
combinations of order and timing. The order classifier was used to decode between
sequences with different finger orders, regardless of their pairing with a timing feature,
whereas the timing classifier was trained to decode between sequences with different
finger timings regardless of their pairing with a specific finger order. These two classifiers
allowed the identification of regions which contained above chance decoding of sequence
order and timing independently of the other sequence feature, respectively (Figure 5a and
Supplementary Figure S2 for t-maps). The integrated classifier decoded residual patterns
after subtracting averaged sequence order and timing related patterns for each run
separately, in order to detect regions which hold information on sequence identity that is
not driven by a simple summation of order and timing information (see Methods).

To reveal the continuous profile of feature decoding along contralateral motor regions on
the cortical surface, we employed the same permutation test approach [29] as in the % signal
change analysis for each of the three classifiers, for preparation and production, separately
(Figure 5b). During preparation, a significant cluster was found for finger order within SPCp
($p = .040$), and a marginally significant cluster for timing decoding was identified within PMv
($p = .054$). During production, above chance decoding was shown for the integrated
classifier within PMd in two clusters ($p = .002$, $p = .044$, on anterior to posterior and ventral
to dorsal cross-sections, respectively) and S1, which extended into M1 and SPCa ($p = .007$).
Above chance decoding of timing was found within SPCa ($p = 0.016$), PMv ($p < .001$), and
SMA ($p = .045$).

Next, we examined how well sequence features could be decoded from pre-registered
ROIs during preparation and production. These regions covered premotor to superior
parietal areas: PMd, PMv, M1, S1, SMA/pre-SMA, SPCa, and SPCp. First, to identify above
chance decoding of sequence information in these areas, one-sample t-tests were
performed on the z-values extracted from each of the pre-defined ROIs during both
preparation and production for timing, order, and integrated classifiers (Figure 5c). These t-
tests were Bonferroni corrected six times, to account for phase (2) by classifier (3) within
each pre-defined ROI. During preparation, the only region that reached significance above
chance was found in SPCp for sequence order decoding ($t(23) = 2.74$, $p = .036$), with
marginally significant decoding also in SPCp for sequence timing ($t(23) = 2.51$, $p = .060$).
During production, classification increased above chance for sequence timing in SMA/pre-
SMA ($t(23) = 2.71$, $p = .036$), PMv ($t(23) = 3.00$, $p = .018$), and SPCa ($t(23) = 2.67$, $p = .042$).
Further, classification increased above chance for order-timing integration in S1 ($t(23) =$
3.69, $p = .003$), PMd ($t(23) = 3.06$, $p = .018$), SPCa ($t(23) = 4.36$, $p < .001$), and SPCp ($t(23) =$
3.20, $p = .012$).

Finally, we set out to test our main hypotheses (osf.io/g64hv) regarding an interaction
between peri-movement phase (preparation, production), classifier (timing, order,
integrated) and region (PMd, PMv, M1, S1, SMA/pre-SMA, SPCa, SPCp). A repeated-
measures ANOVA revealed a significant main effect of phase ($F_{(1,23)}$ = 9.49, p = .005, ηp^2 =
.292), substantiating a general increase of decoding accuracy across regions and classifiers
during production. The main effect of region was not significant ($F(3.84,88.42)$ = 0.45, p =
.763, ηp^2 = .019, Greenhouse-Geisser corrected), suggesting that all the contralateral cortical
ROIs had a comparable contribution to sequence decoding across trial phases. Importantly,
we found a significant phase by classifier interaction ($F(2,46)$ = 10.34, p = .044, ηp^2 = .127),
which was driven by an overall increase in the integrated classifier accuracy from
preparation (M = -0.10, SE = 0.13) to production (M = 0.49, SE = 0.11) (p = .003, $95\% CI$ [.217,
.971], Bonferroni corrected). Finally, there was no significant interaction of phase by region
($F(3.20,73.50)$ = 0.79, p = .512, ηp^2 = .033, Greenhouse-Geisser corrected), or phase with
classifier by region ($F(5.40,124.18)$ = 1.63, p = .151, ηp^2 = .066, Greenhouse-Geisser
corrected). In sum, this supports the hypothesis that tuning of these regions to high and
low-level features of sequences changes dynamically depending on trial phase, rather than
region, with a state shift towards sequence feature integration after movement initiation
across multiple regions.

Figure 5. Multivariate pattern classification results. (a) Inflated surface (upper panels) and flat maps (lower
panels), showing mean decoding z-accuracy values above chance for finger order (blue), timing (red), and
integrated sequence patterns (green). (b) Mean decoding z-accuracy values for each classifier along the cross-
sections explained in Figure 4b. Coloured asterisks denote the respective significant above-chance clusters for
each classifier during preparation and production. (c) Searchlight z-accuracy values were extracted using pre-
determined ROIs shown in the left panel. Decoding above is indicated by the coloured asterisks. The asterisk in
parentheses represents a marginally significant result, p = .060. ** p < 0.01; * p < 0.05, one-sided t-test.

DISCUSSION

Activity in the premotor, primary motor and parietal cortices has been associated with
motor sequence control, from their hierarchical organisation [11,17,22,26,27,31,32] to the control of
spatial and temporal features of sequences [9,12,22,33–35]. Yet how sequence-related
computations in these cortical regions unfold across planning and execution phases remains
uncertain. Do these cortical areas retain a fixed tuning to sequence features and their
integration throughout planning and execution? Or do they switch their content dynamically
depending on whether they occur before or after motor initiation? Here, we examined how
motor cortical areas integrate informational content on sequence features – the order of
finger movement sequences and their timing – across the planning and execution phases.
Sequence decoding from local cortical activity patterns revealed that high-level features of
sequence organisation remain separate during movement planning and are integrated
holistically into unique patterns upon movement initiation in premotor and parietal areas.

Cortical patterns switch their tuning from planning to execution

Our results demonstrate a generalised dependency of cortical representations on peri-
movement phase, with a global shift across regions towards feature integration at the
transition from sequence planning to execution. This indicates that cortical motor-related
areas do not rigidly map onto higher-level versus lower-level representations of sequential
organisation, respectively, as assumed by earlier studies that focussed on activity patterns
during sequence execution alone [12,26,36]. Instead, pattern activity tuning in these regions
changes dynamically upon motor initiation. Such a state switch from higher-level
independent to lower-level integrated control echoes previous findings for the primary
motor and dorsal premotor cortices in the context of single movements. These show that
preparatory neural population activity occupies a different state space (output-null) from
the production activity to prevent readout from downstream areas during planning [11,37,38].
Here, cortical motor planning patterns are not simply subthreshold versions of execution
activity patterns controlled by inhibitory gating within the cortex or downstream as
suggested previously [39,40], but a qualitatively different activity pattern of the neural
population. Our results support the notion of a distinct functional tuning during motor
planning across regions on the premotor to parietal axis in the context of sequential
movements.

Lack of sequence feature integration prior to motor initiation

As participants trained to perform the four finger sequences over two days and entirely
from memory, one may expect that this level of practice would result in their retrieval as
one integrated spatio-temporal synergy [41]. However, we found that information about
motor sequence order and timing of the upcoming sequence was reinstated independently
and integrated after motor initiation only. This recompilation of sequence features occurred
on a trial-by-trial basis. One possibility is that the observed lack of integration during

preparation may be due to requirements of the two-by-two task design, which may
encourage participants to hold onto higher level representations of order and timing.
However, in previous tasks where only one combination of timing and order was trained,
independent transfer of known order and timing to new combinations was still found,
showing that the separation is not dependent on the task structure, but occurs more
generally [5,6].

Although previous work has shown that planning-related activity in motor areas is
predictive of movement features such as speed, force, and trajectory of the upcoming
movement [42–44], these may be regarded as part of planning a holistic motor synergy [45–47]. In
contrast, for sequence learning there is now ample evidence that higher-level sequence
features such as movement order and timing are encoded independently [5,7,12,13] and remain
separate during planning [14,48], despite training across multiple days and production from
memory. This is in line with recent evidence in macaque motor cortex suggesting that the
neural generation of sequence elements with a discrete timing goal – separated by a delay
or in rapid succession – remains independent, despite long-term training and fusion at the
muscular level [11].

Our results show a clear phase-related state shift within regions for discrete movement
sequences features, yet how this integration occurs in more continuous overlapping
movement sequences is unclear. Rather than a dedicated timing system as is observed with
discrete movements [5,12,13,16], continuously overlapping movements have been shown to
employ a more state-dependent timing system [49–52] meaning that they are likely to employ
differing neural mechanisms. Further research should investigate whether sequential
movements with overlapping, continuous trajectories that lack separate timing goals show
the same state shift in informational tuning observed in the current findings.

What triggers sequence feature integration trial-by-trial? We propose that contralateral
motor-related cortical regions activate movement order and timing plans separately until a
sensory stimulus like the Go cue triggers the binding of the corresponding neural patterns.
This binding may occur through subcortical, e.g. thalamic input triggering an appropriate
state for motor execution of specific combination of features [53,54]. In sum, delaying the
binding of sequence features to the production phase and maintaining higher level
separation may allow the system to retain maximum flexibility trial-by-trial, should task
demands change.

Independent patterns for sequence timing are reinstated during execution

We found a stark asymmetry with regard to sequence order and timing during the sequence
production phase. In contrast to the independent patterns for finger order, the activity
patterns tuned to sequence timing became more prominent or emerged during production
in the PMv and SMA/pre-SMA, as well as the superior parietal cortices. Thus, cortical
patterns for sequence timing are reinstated alongside the emergence of sequence-specific
integrated patterns. This asymmetry was also observed at the behavioural level in the
transfer task. Here, trained timing could be quickly recombined with a new finger sequence
producing significant advantages to a sequence that had both new timing and new order in
line with previous work [6,12,14–16]. In contrast, producing the same finger order with a new
timing was associated with a significantly poorer performance. Thus, in contrast to a
previous study utilising the same task paradigm and well-trained sequences produced from

memory [14], here, participants were unable to separate the trained order from their timing.
This interference effect directly parallels the prominence of integrated and the lack of
independent finger order tuning during motor production.

M1 lacks information about sequences despite a large activity increase during execution

Our results show a lack of sequence feature separation or integration in contralateral M1
during preparation and only limited integration above chance during production extending
out from the greater peak in S1. This occurs despite a large activity increase in M1 during
production. While this contrasts with several previous neuroimaging studies [12,19,26,55,56],
recent findings show that information held within M1 is not related to sequence control.
Activity patterns do not change with sequence learning [21,57] and reflect the processing of
individual movements, particularly, the first press of a sequence [20]. In our study, the first
finger press was matched across sequences within participants and the GLM of the BOLD
patterns predicted the response function related to this matched first press only, reducing
the possible influence of subsequent presses. So far, there has been no experimental
evidence that sequential movements are neurally fused in M1 into holistic representations:
Constituent movements remain individuated in M1 regardless of sequential context [11,27].
Therefore, controlling for the first finger press might explain why we see no prominent
sequence feature integration within M1, as observed previously [12].

Extending the previous motor planning framework to sequential actions

The current framework for single movement motor planning proposes that the motor
system enters a preparatory state that is distinct from movement execution and, when
movement is cued, dynamically and passively evolves across a time period in order to
produce movements [37,47,58]. Recent findings also suggest a distinction between the selection
of motor goals and true motor planning, which formulate 'what' movements to execute and
'how' to execute them, respectively [59,60], converging with the idea of hierarchical motor
control [1,26]. In the context of skilled sequence control, we propose that sequence order and
timing features are specified during planning as 'what' elements representing higher-level
control, and integrated during execution as 'how' elements, representing lower-level
implementation motor control. Crucially, our results suggest that individual regions can
undergo a state shift from 'what' to 'how' control depending on the peri-movement phase.
Future electrophysiological research should address whether the same neuronal
populations are involved in both types of control and determine the neural origin and exact
time point that triggers this cortical state shift.

MATERIALS AND METHODS

Participants

24 neurologically healthy participants - 14 females and 10 males (M = 21.00 years, SD =
1.64) - met all behavioural and imaging requirements after completing the three-day
experiment. 23 Participants were right-handed with a mean Edinburgh Handedness
Inventory (EHI; https://www.brainmapping.org/shared/Edinburgh.php; adapted from
Oldfield (1971)) score of 75.22 (SD = 20.97, Range: 25-100), one was left-handed with an EHI
score of -70. Data were collected from an additional 17 participants but were excluded. One
participant was excluded due to unforeseen technical difficulties with the apparatus and

one participant was excluded due to a corrupted functional scan. 15 further participants did
not reach target performance during training and so were also excluded following training.
Target performance consisted of an error rate below 20% (M = 6.54%, SD = 6.03, for the
group) and distinct sequence timing structures. Distinct sequence timing was fulfilled if
there was a significant interval position by sequence timing interaction on IPI duration in
each participant during the fMRI session (Group F(1.78,40.77) = 73.76, p <.001, ηp^2 = .762,
Greenhouse-Geisser corrected, repeated measures ANOVA). Participants were recruited
either through social media and given monetary payment, or through a participation panel
at Bangor University and awarded module credits for their participation. Participants with
professional musical qualifications were excluded from recruitment. All participants
provided informed consent, including consent to data analysis and publication, through an
online questionnaire hosted by Qualtrics (Qualtrics, Provo, UT). This experiment and its
procedures were approved by the Bangor University School of Psychology Ethics Committee
(Ethics approval number 2019-16478).

Apparatus

Force data from fingers of both the right and left hands were recorded at a sample rate of
1000hz using two custom-built force transducer keyboards (10 channels). Each key had a
groove within which the respective fingertip was positioned. A force transducer (Honeywell
FS Series, with a range of up to 15 N) was located under each groove and recorded the
respective finger force without crosstalk between channels. Force data acquisition occurred
in each trial from 500ms before sequence cue onset to the end of the production period in
production trials, and the end of the false production period in No-Go trials. The keys could
be adjusted in position by sliding them up and down individually along the keyboard plane
to achieve the most comfortable position for the hand and wrist when seated during
training or in supine position in the MRI scanner, respectively. Once adjusted the position of
the keys was fixed. Traces from the right hand were baseline-corrected by the first 500ms of
acquisition (500ms before the sequence cue) and smoothed to a Gaussian window of
100ms, trial-by-trial. Button presses were defined as the point at which forces above
baseline exceeded a fixed threshold (2.5 N for the first 8 participants and 1 N for the
subsequent 16 out of 24 participants). Press timings were identified by the timestamp
provided by National Instruments Data Acquisition Software (National Instruments, Austin,
TX) associated with the data point at which the respective threshold was exceeded.

During behavioural training sessions, participants were seated at a wooden table
approximately 75cm away from a 19-inch LCD LG Flatron L1953HR, at a resolution of 1280 x
1024, at a refresh rate of 60Hz. Their hands were occluded by a horizontally positioned
panel on posts around the force boxes. During fMRI sessions, stimuli were presented on an
MR Safe BOLDScreen 24", at a resolution of 1920x1200 and a refresh rate of 60Hz.
Participants laid supine on the scanner bed and the two force transducers were positioned
on a plastic support board resting on their bent upper legs to enable comfortable and stable
positioning of the hands.

Behavioural task

Participants were trained to produce four five-finger sequences with defined inter-press-
intervals (IPI) from memory in a delayed sequence production paradigm. 'Go' trials began
with a fractal image (Sequence cue) presented for 400 milliseconds (ms) which was

associated with a sequence. The mapping between fractal image and each sequence was
defined randomly for each participant. Following the Sequence cue, a fixation cross was
shown to allow participants to prepare the upcoming sequence; display length of this
fixation cross was jittered at durations of 600ms, 1100ms, 1600ms, and 2100ms,
pseudorandomised across trials within blocks. A black hand with a green background (Go
cue) then appeared for 4000ms to cue sequence production. Succeeding the Go cue,
another fixation cross was presented in a jittered fashion at durations of 500ms, 1000ms,
1500ms, and 2000ms. Feedback (see feedback section for more details) was then presented
to participants for 1000ms, followed by a jittered inter-trial-interval (ITI) duration of
1000ms, 1500ms, 2000ms, and 2500ms. Visually guided (Instructed) 'Go' trials during
training were presented in the same fashion albeit featuring a Go cue with a grey
background, and a red dot on the tip of each finger on the hand image would move from
finger to finger in the target production order and in-pace with the target timing structure.
'No-Go' had the same structure to 'Go' trials, but no Go cue was shown succeeding the
preparatory fixation cross. Instead of the Go cue the fixation cross continued to show for an
additional 1000ms. As in 'Go' trials, this phase of the trial was followed by a fixation cross,
feedback and ITI.

Four target sequences consisted of permutations of two finger orders (Order 1 and 2)
and two IPI orders (Timing 1 and 2) matched in finger occurrence and sequence duration.
Sequence orders were generated randomly for each participant. All trained sequences
began with the same finger press to avoid differences in the first press driving the decoding
of sequence identity during preparation [20]. Ascending and descending press triplets and any
identical sequences were excluded. Timing structures were the same across participants, to
allow for comparison of timing performance across participants. The two trained timing
structures consisted of four target IPI sequences as follows: 1200ms-810ms-350ms-650ms
(Timing 1), and 350ms-1200ms-650ms-810ms (Timing 2). To assess if participants
maintained the target timing structure despite individual tendencies to lengthen or
compress overall sequence length, we calculated timing error for each participant relative to
their average total production length. This was calculated offline by normalising target and
produced IPIs as a percentage of the participant's average total sequence length during the
session across sequences, then calculating the cumulative percent deviation from target for
each IPI, averaged across trials.

Feedback was given to participants trial-by-trial on a points-based scale ranging from 0 to
10. Points were based on initiation reaction time (RT) and temporal deviation from target
timing calculated as a percentage of the target interval length. For initiation reaction time,
up to five points were awarded for a fast initiation RT as follows: five points for presses
within 200ms of the Go cue, four points for presses within 200-360ms, three points for
presses within 360-480ms, two points for presses within 480-560ms, one point for presses
within 560-600ms, and zero points for presses beyond 600ms. For IPI performance, up to
five points were awarded based on deviation from target IPI structure in percent of
respective interval to account for the scaling of temporal error with IPI length [62]. Five points
were awarded for average deviations of IPIs from target for each trial which was lower than
10 percent, four points for 10-20 percent, three points for 20-30 percent, two points for 30-
40 percent, one point for 40-50 percent, and zero points for above 50 percent. If the
executed press order was incorrect, participants were awarded 0 points for the trial. If the
executed press order was correct, they were awarded their earned timing points. To

discourage premature key presses in the preparation period of 'Go' trials and 'No Go' trials,
0 points were awarded if participants exceeded a force threshold during preparation above
the baseline period. In No-Go trials, five points were awarded if no press was made as
instructed. A monetary reward of £10 was offered to the two participants who accumulated
the most points across the course of the experiment, to incentivise good performance.

Participants were presented with a feedback screen after each trial showing the number
of cumulative points across the whole experiment, as well as feedback on whether they
pressed the correct finger at the correct time. A horizontal line was placed in the centre of
the screen, with four symbols displayed equidistantly along the line which represented each
of the five finger presses. An 'X' indicated a correct finger press, and a '-' indicated an
incorrect finger press for each sequence position. The vertical position of these symbols
above ("too late") or below ("too early") the line was proportional to the participant's
timing of the respective press relative to target IPI (in %). Using these cues, participants
could adjust their performance online to ensure maximum accuracy of sequence production
and prevent a drift in performance from memory following training. During the first two
days of training, auditory feedback in the form of successive rising tones corresponding to
the number of points (0-10) were played alongside the visual feedback. Auditory feedback
was absent during the fMRI session, to prevent any auditory processing driving decoding
accuracy.

Procedure

Training duration was fixed across participants and occurred across the first two days of the
experiment over three distinct training stages (see Figure 2 for a visual representation of the
training stages). In the first training stage, 80% of all trials were instructed 'Go' trials (black
hand on grey background, Figure 2c), and the remaining 20% were 'No-Go' trials. During the
second training stage, 40% of trials were instructed 'Go' trials, 40% were from-memory 'Go'
trials (black hand on green background, Figure 2c), and 20% were 'No-Go' trials (Figure 2d).
In the third and final stage of training, 80% of trials were from-memory 'Go' trials, and 20%
were 'No-Go' trials. Each stage of training consisted of 240 trials for a total of 720 trials
across all three training sections. The third and final day consisted of a short refresher stage
of 40 trials, made up of the same proportion of trials as the second stage of training, during
which T1 images were collected. Following this refresher stage there was a fMRI stage
consisting of 288 trials (48 trials in each block) featuring 50% from-memory 'Go' trials and
50% 'No-Go' trials.

In addition, before and after the last training stage, participants completed a
synchronisation task during which participants were asked to synchronize their respective
presses to a visual finger cue, as in the first stages of training consisting of four blocks of 32
trials which included trained sequences, sequences with new timings but the same orders
(order transfer), sequences with the same timings but new orders (timing transfer), and new
sequences. Trial structure was identical to instructed 'Go' trials. There were four sequences
belonging to each condition and each sequence was shown for eight consecutive exposures
(Figure 3c) to assess short-term learning gains. We expected that participants would show
significantly more accurate synchronization to visual sequences when they encountered
trained sequences as well as sequences with a trained finger order or trained timing
compared to untrained control sequences following the completion of training.

MRI acquisition

Images were obtained on a Philips Ingenia Elition X 3T MRI scanner using a 32-channel head
coil. T1 anatomical scans were acquired using a magnetisation-prepared rapid gradient echo
sequence (MPRAGE) scan at a 0.937 x 0.937 x 1 resolution, with a field of view of 240 x 240 x
175 (A-P, R-L, F-H), encoded in the anterior-posterior dimension.

T2*-weighted Functional images were collected across six runs of 230 volumes each with
a TR of 2 seconds, a TE of 35ms and a flip angle of 90°. The voxel size was 2mm isotropic, at
a slice thickness of 2mm, with 60 slices. These were obtained in an interleaved odd-even
echo-planar imaging (EPI) acquisition at a multi-band factor of two. Four images were
discarded at the beginning of each run to allow the stabilisation of the magnetic field. The
central prefrontal cortex, the anterior temporal lobe and ventral parts of the cerebellum
were not covered in each participant. Jitters were employed within each trial during
preparation periods, post-production fixation crosses, and inter-trial intervals, to vary which
part of the trial is sampled by each TR and therefore give us a more accurate estimate of the
hemodynamic response function [63].

Pre-processing and first-level analysis

All fMRI pre-processing was completed using SPM12 (Revision 7219) on MATLAB (The
MathWorks, Inc., Natick, MA). Slice timing correction was applied using the first slice as a
reference to interpolate all other slices to, ensuring analysis occurred on slices which
represent the same time point. Realignment and unwarping were carried out using a
weighted least-squares method correcting for head movements using a 6-parameter motion
algorithm. A mean EPI was produced using SPM's 'Imcalc' function, wherein data acquired
across all six runs was combined into a mean EPI image to be co-registered to the
anatomical image. Mean EPIs were co-registered to anatomical images using SPM's 'coreg'
function and their alignment was checked and adjusted by hand to improve the alignment, if
necessary. All EPI runs were then co-registered to the mean EPI image.

For the general linear model (GLM), regressors were defined for each sequence
separately for both preparation and production. Preparation- and production-related BOLD
responses were independently modelled from 'No-Go' and 'Go' trials, respectively, to tease
out activity from these brief trial phases despite given the haemodynamic response lag [64].
The preparation regressor consisted of boxcar function starting at the moment of the
Sequence cue in 'No-Go' trials and lasting for the duration of the maximum possible
preparation phase (2500 ms). The production regressor consisted of a boxcar function
starting at the onset of the first press with a fixed duration of 0 (constant-duration impulse),
to capture activity related to sequence initiation and extract sequence production related
activity from the first finger press that was matched across sequences within each
participant. Additionally, we included regressors or no interest: 1) Error trials (incorrect or
premature presses during 'Go' trials and presses during No-Go trials) which were modelled
from sequence cue onset to the end of the ITI, 2) the preparation period in 'Go' trials (1000-
2500 ms from Sequence cue) and 3) the temporal derivate of each regressor. The boxcar
model was then convolved with the standard hemodynamic response function. To remove
the influence of movement-related artifacts, we used a weighted least-squares approach [65].
The GLM regressors were optimised based on independent pilot data (N=10).

Surface reconstruction

Cortical surface reconstruction was conducted on each participant's T1 anatomical image using Freesurfer's recon-all function [66]. Surface structures were then co-registered to the symmetrical Freesurfer average atlas [67] using surface Caret [68]. Searchlights for multivariate Pattern Analysis (MVPA) were then defined on each individual surface using the node maps provided by the surface reconstruction and displayed in atlas space.

Cross-sectional and region of interest analysis

Two cross-sections were defined upon the cortical surface: 1) anterior to posterior, running from PMd to OPJ and 2) ventral to dorsal, running from PMv to SMA. These cross-sections were taken from a previous study [12]. Data points along these axes were extracted to provide a continuous measure along the cortical surface, which was then subjected to a non-parametric permutation analysis to identify clusters which were significantly above baseline [29]. This was conducted as a one-tailed test, with 10,000 permutations.

Region of interest analysis was conducted using the Caret toolbox [68] on RoIs which were defined based on several previous studies [12,20,21], consisting of PMv, PMd, M1, S1, SMA/pre-SMA, SPCa, and SPCp. Z-values for each classifier were averaged within regions to give an overall value for each decoder, these values were calculated from unsmoothed individual data. One-sample t-tests against chance level (zero) then identified significantly above-chance decoding values on these cross-sections.

Multi-variate pattern analysis of fMRI

Multivariate pattern analysis (MVPA) was conducted using a custom-written MATLAB code to detect sequence-specific representations [12,14]. We used a searchlight of 160 voxels and a maximum searchlight radius of six millimetres. Each searchlight was run on each individual's cortical surface-reconstructed anatomy, projected onto the Freesurfer average atlas [67]. The classification accuracy for each searchlight (cf. classification procedures below) was assigned to the centre of each searchlight. A classification accuracy map was generated by moving the searchlight across the cortical surface [30]. Mean patterns and common voxel-by-voxel co-variance matrices were extracted for each class from training data set (five of the six imaging runs), and then a gaussian linear discriminant classifier was used to distinguish between the same classes in a test data set (the remaining imaging run). For overall sequence classification (Supplementary Figure S1b), the classifier was trained to distinguish between sequences on five runs and then tested on the remaining run, performed on betas estimated from the sequence preparation and production periods independently. Discrimination was then cross-validated across runs (six cross-validation folds).

The factorised classification of finger order, timing, and integrated order and timing followed the previous approach [12]. For the decoding of sequence timing, the classifier was trained to distinguish between two sequences with differing timing but matching order across five runs and was then tested on two sequences with the same two timings paired with a different order in the remaining run. This classification was then cross-validated across runs and across training/test sequences, for a total of 12 cross-validation folds. For the decoding of sequence order, the classifier was trained to distinguish between two sequences of differing orders paired with the same timing and tested on two sequences with the same two orders when paired with a different timing and underwent the same cross-validation procedure. The integrated classifier was analogous to overall sequence decoding, but here the mean activity for each timing (collapsed across two orders) and

finger order (collapsed across two timings) condition within each run was subtracted from
the overall activity for each run, separately. This allowed for the measurement of residual
activity patterns that were not explained by a linear combination of timing and order. For
better comparability across classifiers and for the group analysis, the classification
accuracies were transformed to z-scores, assuming a binomial distribution of the number of
correct guesses. We then tested these z-scores against zero (chance level) on cortical cross-
sections of interest and in pre-defined ROIs across participants for statistical analysis.

REFERENCES

1. Diedrichsen, J. & Kornysheva, K. Motor skill learning between selection and
execution. *Trends in Cognitive Sciences* vol. 19 227–233 (2015).

2. Hikosaka, O., Nakamura, K., Sakai, K. & Nakahara, H. Central mechanisms of motor
skill learning. *Current Opinion in Neurobiology* vol. 12 217–222 (2002).

3. Rosenbaum, D. A., Cohen, R. G., Jax, S. A., Weiss, D. J. & van der Wel, R. The problem
of serial order in behavior: Lashley's legacy. *Hum. Mov. Sci.* **26**, 525–554 (2007).

4. Gobel, E. W., Sanchez, D. J. & Reber, P. J. Integration of Temporal and Ordinal
Information During Serial Interception Sequence Learning. *J. Exp. Psychol. Learn.*
Mem. Cogn. **37**, 994–1000 (2011).

5. Ullén, F. & Bengtsson, S. L. Independent Processing of the Temporal and Ordinal
Structure of Movement Sequences. *J. Neurophysiol.* **90**, 3725–3735 (2003).

6. Kornysheva, K., Sierk, A. & Diedrichsen, J. Interaction of temporal and ordinal
representations in movement sequences. *J. Neurophysiol.* **109**, 1416–1424 (2013).

7. Zeid, O. & Bullock, D. Moving in time: Simulating how neural circuits enable rhythmic
enactment of planned sequences. *Neural Networks* **120**, 86–107 (2019).

8. Calderon, C. B., Verguts, T. & Frank, M. J. Thunderstruck: The ACDC model of flexible
sequences and rhythms in recurrent neural circuits. *PLoS Comput. Biol.* **18**, 1–33
(2022).

9. Merchant, H., Pérez, O., Zarco, W. & Gámez, J. Interval tuning in the primate medial
premotor cortex as a general timing mechanism. *J. Neurosci.* **33**, 9082–9096 (2013).

10. Lafuente, V. de *et al.* Keeping time and rhythm by replaying a sensory-motor engram.
bioRxiv **52**, 1–23 (2022).

11. Zimnik, A. J. & Churchland, M. M. Independent generation of sequence elements by
motor cortex. *Nat. Neurosci.* **24**, 412–424 (2021).

12. Kornysheva, K. & Diedrichsen, J. Human premotor areas parse sequences into their
spatial and temporal features. *Elife* **3**, e03043 (2014).

13. Bengtsson, S. L., Ehrsson, H. H., Forssberg, H. & Ullén, F. Dissociating brain regions
controlling the temporal and ordinal structure of learned movement sequences. *Eur.*
J. Neurosci. **19**, 2591–2602 (2004).

14. Kornysheva, K. *et al.* Neural Competitive Queuing of Ordinal Structure Underlies
Skilled Sequential Action. *Neuron* **101**, 1166-1180.e3 (2019).

15. O'Reilly, J. X., McCarthy, K. J., Capizzi, M. & Nobre, A. C. Acquisition of the temporal
and ordinal structure of movement sequences in incidental learning. *J. Neurophysiol.*
99, 2731–2735 (2008).

16. Shin, J. C. & Ivry, R. B. Concurrent Learning of Temporal and Spatial Sequences. *J. Exp.*
Psychol. Learn. Mem. Cogn. **28**, 445–457 (2002).

17. Kennerley, S. W., Sakai, K. & Rushworth, M. F. S. Organization of Action Sequences

and the Role of the Pre-SMA. *J. Neurophysiol.* **91**, 978–993 (2004).

18.   Tanji, J. & Shima, K. Role for supplementary motor area cells in planning several
movements ahead. *Nature* **371**, 413–416 (1994).

19.   Wiestler, T. & Diedrichsen, J. Skill learning strengthens cortical representations of
motor sequences. *Elife* **2013**, 801 (2013).

20.   Yokoi, A., Arbuckle, S. A. & Diedrichsen, J. The role of human primary motor cortex in
the production of skilled finger sequences. *J. Neurosci.* **38**, 1430–1442 (2018).

21.   Berlot, E., Popp, N. J. & Diedrichsen, J. A critical re-evaluation of fmri signatures of
motor sequence learning. *Elife* **9**, 1–24 (2020).

22.   Wiestler, T., Waters-Metenier, S. & Diedrichsen, J. Effector-independent motor
sequence representations exist in extrinsic and intrinsic reference frames. *J. Neurosci.*
34, 5054–5064 (2014).

23.   Picard, N., Matsuzaka, Y. & Strick, P. L. Extended practice of a motor skill is associated
with reduced metabolic activity in M1. *Nat. Neurosci.* **16**, 1340–7 (2013).

24.   Matsuzaka, Y., Picard, N. & Strick, P. L. L. Skill representation in the primary motor
cortex after long-term practice. *J. Neurophysiol.* **97**, 1819–32 (2007).

25.   Wymbs, N. F., Bassett, D. S., Mucha, P. J., Porter, M. A. & Grafton, S. T. Differential
Recruitment of the Sensorimotor Putamen and Frontoparietal Cortex during Motor
Chunking in Humans. *Neuron* **74**, 936–946 (2012).

26.   Yokoi, A. & Diedrichsen, J. Neural Organization of Hierarchical Motor Sequence
Representations in the Human Neocortex. *Neuron* **103**, 1178-1190.e7 (2019).

27.   Russo, A. A. *et al.* Neural Trajectories in the Supplementary Motor Area and Motor
Cortex Exhibit Distinct Geometries, Compatible with Different Classes of
Computation. *Neuron* **107**, 745-758.e6 (2020).

28.   Ariani, G., Pruszynski, J. A. & Diedrichsen, J. Motor planning brings human primary
somatosensory cortex into action-specific preparatory states. *Elife* **11**, (2022).

29.   Maris, E. & Oostenveld, R. Nonparametric statistical testing of EEG- and MEG-data. *J.*
Neurosci. Methods **164**, 177–190 (2007).

30.   Oosterhof, N. N., Wiestler, T., Downing, P. E. & Diedrichsen, J. A comparison of
volume-based and surface-based multi-voxel pattern analysis. *Neuroimage* **56**, 593–
600 (2011).

31.   Sakai, K., Kitaguchi, K. & Hikosaka, O. Chunking during human visuomotor sequence
learning. *Exp. Brain Res.* **152**, 229–242 (2003).

32.   Gerloff, C., Corwell, B., Chen, R., Hallett, M. & Cohen, L. G. Stimulation over the
human supplementary motor area interferes with the organization of future elements
in complex motor sequences. *Brain* **120**, 1587–1602 (1997).

33.   Shima, K. & Tanji, J. Both supplementary and presupplementary motor areas are
crucial for the temporal organization of multiple movements. *J. Neurophysiol.* **80**,

3247–3260 (1998).

34.   Ramnani, N. & Passingham, R. E. Changes in the Human Brain during Rhythm
Learning. *J. Cogn. Neurosci.* **13**, 952–966 (2001).

35.   Crowe, D. A., Zarco, W., Bartolo, R. & Merchant, H. Dynamic representation of the
temporal and sequential structure of rhythmic movements in the primate medial
premotor cortex. *J. Neurosci.* **34**, 11972–11983 (2014).

36.   Diedrichsen, J., Wiestler, T. & Krakauer, J. W. Two distinct ipsilateral cortical
representations for individuated finger movements. *Cereb. Cortex* **23**, 1362–1377
(2013).

37.   Kaufman, M. T., Churchland, M. M., Ryu, S. I. & Shenoy, K. V. Cortical activity in the
null space: Permitting preparation without movement. *Nat. Neurosci.* **17**, 440–448
(2014).

38.   O'Shea, D. J. & Shenoy, K. V. The Importance of Planning in Motor Learning. *Neuron*
vol. 92 669–671 (2016).

39.   Cisek, P. & Kalaska, J. F. Neural correlates of reaching decisions in dorsal premotor
cortex: specification of multiple direction choices and final selection of action. *Neuron*
45, 801–814 (2005).

40.   Duque, J. & Ivry, R. B. Role of corticospinal suppression during motor preparation.
Cereb. Cortex **19**, 2013–2024 (2009).

41.   Gentner, R. *et al.* Encoding of motor skill in the corticomuscular system of musicians.
Curr. Biol. **20**, 1869–1874 (2010).

42.   Yang, L., Leung, H., Plank, M., Snider, J. & Poizner, H. EEG activity during movement
planning encodes upcoming peak speed and acceleration and improves the accuracy
in predicting hand kinematics. *IEEE J. Biomed. Heal. Informatics* **19**, 22–28 (2015).

43.   Pearce, T. M. & Moran, D. W. Strategy-dependent encoding of planned arm
movements in the dorsal premotor cortex. *Science (80-.).* **337**, 984–988 (2012).

44.   Wong, A. L., Goldsmith, J. & Krakauer, J. W. A motor planning stage represents the
shape of upcoming movement trajectories. *J. Neurophysiol.* **116**, 296–305 (2016).

45.   D'Avella, A., Saltiel, P. & Bizzi, E. Combinations of muscle synergies in the construction
of a natural motor behavior. *Nat. Neurosci.* **6**, 300–308 (2003).

46.   Overduin, S. A., D'Avella, A., Roh, J., Carmena, J. M. & Bizzi, E. Representation of
muscle synergies in the primate brain. *J. Neurosci.* **35**, 12615–12624 (2015).

47.   Shenoy, K. V., Sahani, M. & Churchland, M. M. Cortical control of arm movements: A
dynamical systems perspective. *Annual Review of Neuroscience* vol. 36 337–359
(2013).

48.   Mantziara, M., Ivanov, T., Houghton, G. & Kornysheva, K. Competitive state of
movements during planning predicts sequence performance. *J. Neurophysiol.* **125**,
1251–1268 (2021).

49. Kornysheva, K. Encoding temporal features of skilled movements-what, whether and
how? in *Advances in Experimental Medicine and Biology* vol. 957 35–54 (Springer
New York LLC, 2016).

50. Ivry, R. B. & Spencer, R. M. C. The neural representation of time. *Current Opinion in*
Neurobiology vol. 14 225–232 (2004).

51. Ivry, R. B. & Schlerf, J. E. Dedicated and intrinsic models of time perception. *Trends in*
Cognitive Sciences vol. 12 273–280 (2008).

52. Diedrichsen, J., Criscimagna-Hemminger, S. E. & Shadmehr, R. Dissociating timing and
coordination as functions of the cerebellum. *J. Neurosci.* **27**, 6291–6301 (2007).

53. Inagaki, H. K. *et al.* A midbrain-thalamus-cortex circuit reorganizes cortical dynamics
to initiate movement. *Cell* **185**, 1065-1081.e23 (2022).

54. Wang, J., Narain, D., Hosseini, E. A. & Jazayeri, M. Flexible timing by temporal scaling
of cortical responses. *Nat. Neurosci.* **21**, 102–112 (2018).

55. Wymbs, N. F. & Grafton, S. T. The human motor system supports sequence-specific
representations over multiple training-dependent timescales. *Cereb. Cortex* **25**, 4213–
4225 (2015).

56. Nambu, I. *et al.* Decoding sequential finger movements from preparatory activity in
higher-order motor regions: A functional magnetic resonance imaging multi-voxel
pattern analysis. *Eur. J. Neurosci.* **42**, 2851–2859 (2015).

57. Berlot, E., Popp, N. J., Grafton, S. T. & Diedrichsen, J. Combining Repetition
Suppression and Pattern Analysis Provides New Insights into the Role of M1 and
Parietal Areas in Skilled Sequential Actions. *J. Neurosci.* **41**, 7649–7661 (2021).

58. Churchland, M. M., Cunningham, J. P., Kaufman, M. T., Ryu, S. I. & Shenoy, K. V.
Cortical Preparatory Activity: Representation of Movement or First Cog in a
Dynamical Machine? *Neuron* **68**, 387–400 (2010).

59. Wong, A. L., Haith, A. M. & Krakauer, J. W. Motor planning. *Neuroscientist* vol. 21
385–398 (2015).

60. Haith, A. M. & Bestmann, S. *Preparation of Movement. The Cognitive Neurosciences*
VI. Eds: Poeppel, Mangun, Gazzaniga
http://www.bestmannlab.com/images/uploads/Preparation_of_Movement_Haith_B
estmann_FINAL.pdf (2018).

61. Oldfield, R. C. The assessment and analysis of handedness: The Edinburgh inventory.
Neuropsychologia **9**, 97–113 (1971).

62. Rakitin, B. C. *et al.* Scalar expectancy theory and peak-interval timing in humans. *J.*
Exp. Psychol. Anim. Behav. Process. **24**, 15–33 (1998).

63. Serences, J. T. A comparison of methods for characterizing the event-related BOLD
timeseries in rapid fMRI. *Neuroimage* **21**, 1690–1700 (2004).

64. Logothetis, N. K. The underpinnings of the BOLD functional magnetic resonance
imaging signal. *Journal of Neuroscience* vol. 23 3963–3971 (2003).

65.   Diedrichsen, J. & Shadmehr, R. Detecting and adjusting for artifacts in fMRI time
845   series data. *Neuroimage* **27**, 624–634 (2005).

846   66.   Dale, A. M., Fischl, B. & Sereno, M. I. Cortical surface-based analysis: I. Segmentation
847   and surface reconstruction. *Neuroimage* **9**, 179–194 (1999).

848   67.   Fischl, B., Sereno, M. I., Tootell, R. B. H. & Dale, A. M. High-resolution intersubject
849   averaging and a coordinate system for the cortical surface. *Hum. Brain Mapp.* **8**, 272–
850   284 (1999).

851   68.   Van Essen, D. C. *et al.* An integrated software suite for surface-based analyses of
852   cerebral cortex. *Journal of the American Medical Informatics Association* vol. 8 443–
853   459 (2001).

854