A Parcellation Scheme of Mouse Isocortex Based on Reversals in Connectivity Gradients

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Abstract

The brain comprises several anatomically clearly separated structures. This parcellation is often extended into the isocortex, where border demarcations are less clear due to its relatively homogeneous structure. Yet, established parcellation schemes exist, based on anatomical, physiological or functional differences. Here, we derive a parcellation scheme based purely on connectomics, that is, the spatial structure of long-range synaptic connections within the cortex. To that end, we analyze a publicly available dataset of average mouse brain connectivity, and split the isocortex into disjunct regions. Instead of clustering connectivity based on similarity or modularity, our scheme is inspired by methods that split sensory cortices into subregions where gradients of neuronal response properties, such as the location of the receptive field, reverse. We developed a method to calculate comparable gradients from voxelized brain connectivity data and automatically detect reversals in them. This approach better respects the known presence of functional gradients within brain regions than clustering-based approaches. Placing borders at the reversals resulted in a parcellation into 41 subregions that differs significantly from an established scheme in nonrandom ways, but is comparable in terms of the modularity of connectivity between regions. It revealed unexpected trends of connectivity, such a a tripartite split of somato-motor regions along an anterior to posterior gradient. The method can be readily adapted to other organisms and data sources, such as human functional connectivity.

1 Introduction

Established parcellation schemes of the cortex (Zilles and Amunts, 2010; Amunts and Zilles, 2015; Sporns, 2015) use anatomical differences - such as presence of a layer 4 - or functional differences - such as responding to certain modalities with low delay - to draw borders between regions. Connections from other brain structures - such as innervation from different thalamic nuclei - also play a role, but connectivity within cortex is typically analyzed with respect to a prior parcellation scheme (Scannell et al., 1995; Bota et al., 2015). Implicit in this is the assumption that the prior scheme is useful in revealing the structure of connectivity. This assumption is not unwarranted, as the observed functional differences are at least partially the result of the intracortical connectivity, in the sense that differences in functional behavior of neurons across regions is likely to be mirrored by differences in connectivity (van den Heuvel et al., 2015). However, the details of parcellation schemes can quantitatively affect the results and consequently make comparison across studies difficult (de Reus and van den Heuvel, 2013). Therefore, this logic has been reversed, splitting the cortex into regions based on its connectivity (Tittgemeyer et al., 2018; Eickhoff et al., 2015). Then, function or anatomy can be analyzed with respect to the results.

This endeavor requires two things: A data source describing the structure of intracortical connectivity, and a way to find and draw borders between spatially compact regions.For the data source, we used the average mouse brain connectome published by the Allen Institute (Oh et al. (2014); Knox et al. (2019), connectivity.brain-map.org, github.com/AllenInstitute). It is at this point the most comprehensive source of information on structural mouse brain connectivity. Further, we have previously demonstrated that it is of sufficient quality to describe the spatial structure of connectivity in terms of pathway strengths, layer profiles and topographical mapping, with respect to a prior brain parcellation (Reimann et al., 2019). Nevertheless, our results must be interpreted with the caveat that

they may be affected by inaccuracies in this source material - the output can only be as accurate as the input. To that end, we ensure that our algorithms are general enough to be readily applied to future, improved data sources. This includes data sources for different organisms, such as human functional connectivity.

A wealth of clustering algorithms exist that could use the connectivity data as an input and prove a parcellation that optimizes a measure such as similarity of connectivity within a region. Such an approach was typically used in previous publications on connectivity based parcellation (Craddock et al., 2012; Eickhoff et al., 2015; Tittgemeyer et al., 2018). Here, however, we developed an alternative method inspired by existing data analysis techniques that find borders between regions in sensory cortices. These techniques consider gradients of the locations of receptive fields associated with cortical locations and draw borders between regions where sudden reversals of gradients are observed (Sereno et al., 1994; Garrett et al., 2014; Schönwiesner et al., 2015; Juavinett et al., 2017). To find analogous gradients in connectivity data, we used a technique called diffusion embedding to detect the strongest gradients in the similarity structure of the voxelized connectome. We found that similar gradient reversals were present in that data that could be automatically detected to determine borders between regions. Crucially, the technique could be readily extended to non-sensory cortices, where the activity-based technique would fail. Eickhoff et al. (2015) pointed out that cortical regions are often functionally organized around gradients (Wandell et al., 2007; Hensel et al., 2015) and that similarity clustering tends to cut borders into them. Our approach avoids this potential issue as it places borders at reversals instead of continuous sections of gradients.

1.1 Motivation and approach

Established techniques draw borders between sensory cortical regions by considering the activity of neurons at various locations. These neurons, and by extension their cortical locations, can be characterized in terms of properties of their preferred stimuli (Sereno et al., 1994; Garrett et al., 2014; Schönwiesner et al., 2015; Juavinett et al., 2017). For some properties, this comes in the form of a continuous topographical mapping, meaning that the entire spectrum of values of the property can be associated with specific cortical locations, with nearby locations being associated with similar values. A property can be represented this way several times in neighboring cortical regions, such as sound frequency being represented in primary auditory cortex (Schönwiesner et al., 2015) or the visual field (retinotopy) being mapped to primary and higher-order visual cortices (Sereno et al. (1994); Garrett et al. (2014); Juavinett et al. (2017); Fig. 1A). At the border between these regions, we cross from one continuous map to another, yet there is no sudden jump in the value of the property, but rather a gradient reversal (Fig. 1B, black arrows). This means that the maps of neighboring regions associated with the same modality are mirror images of each other, which can be used to detect borders between regions. Note that Garrett et al. (2014); Juavinett et al. (2017) specifically use a change of the sign of the gradient of a two-dimensional mapping (horizontal and vertical retinotopy) to detect borders (Fig. 1B, red and blue outlines), but most of the time this change arises from a reversal of one gradient while the other remains constant

We hypothesize that even in the absence of activity recordings, the gradient reversal and thus the border between regions can be detected when considering the connectivity of neurons instead. This is based on the idea that it is the afferent connectivity of neurons, i.e. their input, that determines the quality of their preferred stimulus. Further, neurons with similar preferences have been demonstrated to connect strongly to each other (Rossi et al., 2020; Harris and Mrsic-Flogel, 2013), indicating that also their targets of synaptic outputs are similar. Thus, we attempted to detect gradients in the profiles of afferent and efferent connectivity of individual voxels in the Allen Institute's voxelized mouse connectome.

A technique to find such gradients, diffusion embedding (Vos de Wael et al., 2020), has been used on this dataset before to characterize it (Coletta et al., 2020). Briefly, it positions every voxel in an n-dimensional coordinate system, such that voxels with similar connectivity profiles (i.e. receiving inputs from the same locations and sending outputs to the same locations) are placed more closely to each other (Fig. 1C; for details, see Supplementary Methods, Fig. S1 and (Vos de Wael et al., 2020)). This process allows to reveal embedded geometric structure of connectivity within the data. Each dimension of this coordinate system corresponds to a *component* of connectivity with components placed in order of their strength. In that regard, it can be thought of as similar to principal component analysis.

Previous research using this technique indicates that the difference between sensory modalities forms one strong gradient in the dataset (Coletta et al., 2020). This indicates that the principle of gradient reversal might be useful

not merely to split apart sensory regions of the same modality, but also different modalities and even sensory regions from non-sensory associative areas.

1.2 Gradient reversals in visual regions

To test our hypothetical approach, we first investigated whether the well-established gradient reversals in visual cortices can be recreated from the voxelized connectivity. To that end, we had to give the output of the diffusion embedding a spatial context that could be used to determine its gradients. We used a *flat map* of mouse somatosensory regions, created as described in Bolanos-Puchet and Reimann (2022), that associated each connectivity voxel with a discrete location in a two-dimensional grid. Voxels along an axis orthogonal to cortical layers were mapped to the same location that we refer to as a *pixel*. At a voxel resolution of $100\mu m$, 13 ± 8 (mean $\pm$ std) voxels were mapped to the same pixel. For each pixel, we considered the mean values of the diffusion embedding coordinates of the voxels mapped to that pixel (Fig. 1D). We could then calculate the gradient of any diffusion embedding coordinate along the x- and y-axis of the pixelized image of isocortex (Fig. 1E, F).

This approach explicitly "flattened away" the cortical layers, and it is known that the laminar structure decidedly shapes connectivity (Felleman and Van Essen, 1991). However, we were interested in a parcellation orthogonal to layer boundaries, similar to existing parcellations and in accordance with the theory of the cortical column, i.e. a piece of cortex spanning all layers acting as a functional unit. We characterized the amount of information lost through averaging by comparing the spread of diffusion embedding coordinates of voxels mapped to the same pixel to the one over the mean values of pixels in the same region (Fig. S2). We found that the standard deviation of values within a pixel was almost two orders of magnitude below the standard deviation over a region, demonstrating that the connectivity profiles of voxels along a cortical column are likely similar, thus avoiding too much information through flattening. Yet, in the future our algorithms might be extended by additionally considering a third gradient of a diffusion embedding coordinate along the depth-axis.

We applied this approach to the voxels associated with visual areas in the Allen Institute Common Coordinate Framework (AIBS CCF, Wang et al. (2020), atlas.brain-map.org, Fig. 1D-F). We found in the two strongest components (from here on called α and β) several gradient reversals that roughly coincide with the established parcellation. In the α component we found reversals at the border between VISam and VISpm, splitting VISrl from VISa and VISal, and a number of reversals splitting VISal, VISl and VISli from the rest. In the β component we found a local maximum, leading to a reversal when crossed in any direction, at the point where VISp, VISpm, VISam, VISa and VISrl meet. Additionally, reversals split VISa, VISrl and VISal from the rest. Crucially, the large area of the primary visual cortex (VISp) was not split up by reversals, instead depicting a *continuous mapping* characterized by only smooth changes in the direction of both the α and β gradients.

We conclude that the diffusion embedding coordinates of voxelized connectivity contain similar gradients and gradient reversals as the functional data based on neuron activity. As such, it may be possible *in principle* to build a parcellation based on it.

2 Methods

2.1 Two methods to split regions based on connectivity gradients

We implemented two approaches to splitting regions based on connectivity gradients: *cosine distance clustering* and *reversal detection.* The first generalizes the process of Campello et al. (2013) by considering the angle between a pair of gradients, then clustering them based on similarity, the second one explicitly determines pixels of the flattened view where a gradient reverses.

Both begin by applying diffusion embedding (Vos de Wael et al., 2020) to the matrix of directed connection strengths between voxels, extracting the 20 strongest components (Fig. 2A, left). As discussed in the introduction and Fig. 1, we work in a flattened view of the volume of interest; as such we average the value of each component over the voxels mapped to the same pixel. We then calculate their gradients with respect to the grid of pixels. The next steps differ between the two approaches.

Figure 1: **Parcellation at gradient reversals.** A: Horizontal and vertical retinotopy of mouse visual regions as measured by Juavinett et al. (2017). Data digitized from the original publication. B: Gradients of the retinotopies (black arrows). Overlaid are region with positive sign (smallest rotation from horizontal to vertical gradient is clockwise, red) and with negative sign (smallest rotation is counter-clockwise, blue). Green arrows denote examples of switches of the sign by a sudden reversal of one gradient. C: Diffusion embedding. Build a similarity matrix based on the connectivity strength of considered voxels and run diffusion process on this matrix to extract the embedded geometrical space of connectivity. Extract then the first two dominant eigenvectors of the diffusion distance indicating the connectivity 'profile' of the voxels. D: Left: Flattened view of mouse visual cortex. Subregions according to AIBS CCF indicated in different colors. Right: For each pixel of the flat view we average the first two diffusion coordinates (α and β) of the voxels mapping into the pixel. E: Resulting mean α and β. F: Gradients of the mean α (top) and β (bottom). Red lines indicate manually annotated borders draw at gradient reversals.

Figure 2: **Parcellation methods and evaluation in a toy model of connectivity** A: Symbolic illustration of the workflow. Input is the matrix of connection strengths between voxels of the region to parcellate. The 20 strongest components are extracted through diffusion embedding and gradients are calculated in a flattened view (four gradients indicated). An initial parcellation is derived with one of two methods. Top: A gradient is selected, based on minimizing the reversal index of the resulting parcellation, and a border map is built by convolving the normalized gradient with a uniform kernel. Pixels where the length of the convolved gradient is below 0.97 are classified as border. Distance between a pair of pixels is calculated as the number of border pixels on the path between them using the Dijkstra algorithm. An initial parcellation is generated through Ward linkage. Bottom: For each gradient pairwise cosine distances of the direction of the gradient are calculated. They are summed with weights corresponding to the strength of the respective gradient. An initial parcellation is generated by the HDBSCAN algorithm. Finally, the initial parcellation is post-processed. B: A toy model of connectivity for evaluation of the algorithm. A hierarchical parcellation of a cubic volume is constructed by successively splitting volumes along an axis into n subvolumes (here for resolution $n = 2$ and depth $d = 2$). Right: The value of the strongest connectivity component is then prescribed as a linear gradient inverting at each border. Connectivity is then based on similarity of the prescribed connectivity components. C: The method yields one connection matrix at each hierarchy level. We construct a merged matrix by either multiplying the matrices at all levels (*reversing hierarchy model*, C1), or by considering the matrix at the lowest level and dividing the values in individual submatrices by the path distance between the nodes they represent in the hierarchy graph (*node distance model*, B2, distances from $\alpha_{0,0}$ indicated in yellow). D: Connection matrices of the two models with low ($\phi = 0.1$) and high ($\phi = 5$) noise added.

Cosine distance clustering (Fig. 2A, bottom) considers the gradients of the strongest twenty components and directly calculated a distance metric based on them. For each pair of pixels, a weighted sum of cosine similarities of the gradients was considered, where the weight was equal to the strength of the associated component.

First the gradient of the nth component (ω_n) at a location i was normalized (as in Fig. 1F:

$$\nabla^i_{\omega_n} = \left(\frac{\Delta\omega^i_n}{\Delta x}, \frac{\Delta\omega^i_n}{\Delta y} \right); \hat{\nabla}^i_{\omega_n} = \frac{\nabla^i_{\omega_n}}{\left|\nabla^i_{\omega_n}\right|} \tag{1}$$

Then the weighted sum of cosine similarities was calculated:

$$S^{i,j}_{\omega_n} = \sum_{n=1}^{20} w_n \cdot \hat{\nabla}^i_{\omega_n} \cdot \hat{\nabla}^j_{\omega_n} \tag{2}$$

This was then converted to a distance by subtracting the value from the maximum possible value

$$D^{i,j}_{\omega_n} = \sum_{n=1}^{20} w_n - S^{i,j}_{\omega_n} \tag{3}$$

We then applied the HDBSCAN algorithm (Campello et al., 2013), resulting in a hierarchical clustering that yields an initial parcellation.

Reversal detection (Fig. 2A, bottom) considered the normalized gradient of a single component in its flattened view, $\hat{\nabla}_{\omega_n}$, as above. We calculated the degree of reversal at each location by convolving the gradient field with a two-dimensional Gaussian kernel. If gradients around a pixel have the same orientation, the vector resulting from the convolution at that point will also have unit length; conversely, a reversal would lead to gradients with inverted orientation cancelling each other out in the convolution. We considered a convolved vector shorter than 0.97 to indicate that the location was part of a border. We then determined contiguous regions encircled by the same boundary in the following way: We began by building a graph where each node represented a pixel and edges were placed between all pairs of neighboring pixels (direct or diagonal neighbors). The length of an edge was 1 if either of the pixels was tagged as a border, 0 otherwise. We calculated distances between all pixels as the length of the shortest path in the graph between the pair, as calculated by the Dijkstra algorithm (Dijkstra and others, 1959). Finally, we generated groups of pixels by running the Ward linkage algorithm on the matrix of pairwise distances. We chose the number of clusters between 2 and 10 by optimizing the resulting silhouette score.

Unfortunately, reversals might not be observed equally on every diffusion component, so a first operation is to determine which component to use to perform the reversal detection. While an intuitive choice may be the first, i.e. strongest, component, in practice we found that: 1) This component was not guaranteed to yield the most useful split; and 2) the following components often had very similar strengths, indicating that their order may be partially arbitrary. Consequently, we decided to run the algorithm on all of the 20 strongest components and choose the one that minimizes the *reversal index*, ri within the resulting subregions. Note that in actual biological data, the 20th component still had a strength of 10% of the first component.

ri of a subregion κ is defined as:

$$ri_{\omega,\kappa} = \frac{\sum_{i,j \in \kappa} \left| D^{i,j}_\omega > 90 \right|}{N_\kappa}, \tag{4}$$

where N_κ refers to the number of pixels in κ. The measure counts the fraction of pairwise distances above 90 degrees, indicating of reversals. Thus, the optimization procedure is expressed by:

$$\omega^* = \arg\min_\omega \frac{\sum_{\kappa_i}^m ri_{\omega,\kappa_i}}{m} \tag{5}$$

where m is the number of resulting subregions when a split is applied based on ω.

Both approaches had their advantages and disadvantages. *Reversal detection* considered only one component at a time, requiring the selection heuristic. Also, its convolution step left a number of pixels at the borders of the region unlabelled (Fig. 2A, top right). *Cosine distance clustering*, while considering several components together, did not explicitly seek out reversals, but rather considered absolute differences in gradients. Results also tended to be noisier, and its use of HDBSCAN potentially left a number of pixels classified as outliers and thus unlabelled (Fig. 2A, bottom right).

2.2   Post-processing the initial split

The shortcomings of both methods required a number of post-processing steps (Fig. 2A, right). First, unlabelled pixels (see above) needed to be classified. To that end, we train a Support Vector Machine to classify the unlabelled pixels based on their x and y coordinates in the flat coordinate system (Fig. S3A). This step serves not only to extrapolate the first classification, but also to generalize the output to a less noisy result. Indeed, due to potential noise in the input data, the resulting parcellation of the first gradient classification can be irregular and scattered, especially for *cosine distance clustering*. Second, at this stage all pixels are classified but some clusters of the same class can be spatially non-continuous, therefore these clusters must be differentiated. This is done by hierarchical clustering of pixels of the same class based on their Euclidean distance (Fig. S3B). Third, we "unflatten" the resulting parcellation from pixels to voxels by looking up the reverse images of each pixel (Fig. S3C). Finally, we specify a minimum size threshold for the resulting regions to reject any regions that are unrealistically small and merge them with their closest neighbour (Fig. S3D).

2.3   Evaluating a parcellation

In order to evaluate a parcellation quantitatively, we considered what the gradients of an idealized atomic region would look like (assuming that such a thing exists in the actual connectome). Without gradients related to region differences, we can assume that the only remaining ones would be related to the local connectivity. Its known distance dependence (Petersen and Sakmann, 2000; Lubke, 2003; Holmgren et al., 2003; Perin et al., 2011) can then be assumed to result in gradients that simply reflect the spatial locations of the voxel. In the flat view, this would result in two continuous (i.e. non-reversing) and orthogonal gradients. To measure how close a region comes to this theoretical ideal, we introduce two metrics: the *gradient deviation*, gd that evaluates the orthogonality of the gradient, which is calculated by:

$$gd = |\lambda - 90| \tag{6}$$

where λ is the angle between the two strongest gradients. The second metric evaluates the continuity of the connectivity structure. It is simply the sum of reversal indices of the two strongest components, as defined in equation 4: $ri_\alpha + ri_\beta$.

To test our intuition of orthogonal and non-reversing gradients in the actual biological data, we evaluated the two strongest gradients of an exemplary region (SSp-ll, the lower limb region of primary somatosensory cortex) in different contexts: As part of the entire isocortex (Fig. S4A), the somatosensory and motor areas (same figure, panel B), somatosensory areas (panel C) and individually (D). Note that the values of α and β are in arbitrary units and consequently their sign is arbitrary as well. This means that only the orientations of gradients and locations of reversals are meaningful, but not their direction. As such, results from the level of isocortex down to somatosensory areas are very similar, only once SSp-ll is considered in isolation does β form a second, orthogonal gradient. Consequently values of gd decrease significantly over scales (Fig. S4E), as expected. While ri is actually lowest at the scale of somatosensory areas and increases slightly for SSp-ll in isolation, the reduction relative to the entire isocortex are still substantial.

We conclude that these metrics can be used to test whether the application of a split improves a solution by moving it closer to the theoretically derived ideal. Consequently, they can be used as an indication that a proposed split should be accepted or rejected.

2.4   Recursive repetition of the splitting algorithm

The results in Fig. S4 also demonstrate that gradients can differ substantially depending on the context, i.e. on which parts of cortex were subjected to diffusion embedding together. Intuitively, this is easy to understand: A large-scale connectivity trend, spanning the entire isocortex, such as the one described by component α in Fig. S4A, will not depict its full range of values when evaluated over a small patch. Consequently it will appear weaker and may even be lost to noise. Conversely, a trend with a higher spatial frequency would be less affected. This indicates that also reversals may appear or disappear depending on the spatial context and scale. As such, we may not be able to discover all viable subregions at once in a single execution of the algorithm. However, repeating the algorithm, but separately for each resulting subregion, may reveal further subdivisions. We continue to recursively apply splitting algorithms to each subregion, thereby building not only a parcellation but also a tentative hierarchy. The process is stopped once it becomes apparent that further repetitions do no longer improve the quality of the parcellation.

2.5 Evaluating reversals in an artificial connectome

With these methods, gradient reversals could be detected in any and every part that is covered by the data set. This includes regions outside primary sensory regions, where parcellation based on neuron responses cannot be readily used.

Still, it is unclear to what degree the methods are capable of recovering a true parcellation and how we should interpret its results. We therefore set out to better understand how the procedure works on connectivity data with various, interacting gradients. To that end, we developed a simplified toy model of connectivity based on a prior parcellation that allowed us to evaluate the result against a known ground truth. To build such a model, we had to make strong assumptions about the structure of connectivity that may be inaccurate. Yet, the use of such a model allowed us to evaluate the algorithmic details of parcellation based on gradient reversal detection, such as its resistance against noise. Furthermore, it also improved the interpretation of the results by outlining the limitations of the resulting algorithms.

We build the connectome inside a voxelized 3-d cube, with a regular grid of a given resolution and depth specifying a spatially nested hierarchy of regions. Each level of the hierarchy split the cube along one axis, alternating between the y- and z-axis (Fig. 2B). Connection strengths were generated for a hierarchy level by reversing the diffusion process. We prescribed continuous and reversing target values of the two strongest components, α and β, i.e. attributing increasing – or decreasing – component values to voxels and reversing these components where a different region starts (Fig. 2B, right). E.g. for a split along the y-axis:

$$\alpha(x, y, z) = 2 \left| y \cdot \frac{n}{2} - \left\lfloor y \cdot \frac{n}{2} + 0.5 \right\rfloor \right| ; \beta(x, y, z) = z, \tag{7}$$

where n is the *resolution* of the model, i.e. the number of subregions in the hierarchy level.
The connection strength between each pair of voxels i and j was then defined based on Euclidean distance of those values:

$$S(i, j) = \sqrt{(\alpha(x_i, y_i, z_i) - \alpha(x_j, y_j, z_j))^2 + (\beta(x_i, y_i, z_i) - \beta(x_j, y_j, z_j))^2}, \tag{8}$$

$$C(i, j) = e^{-\sqrt{\frac{S(i,j)}{2 \cdot \sigma^2}}} + n(\phi), \tag{9}$$

where σ was set to 0.1 times the maximum of $S(x, y)$ and $n(\phi)$ denotes noise with a uniform distribution between $-\phi$ and ϕ that was added to test the resistance against noise.

This process could be applied at a given level of the hierarchy to connect the subvolumes at that level of the hierarchy (Fig. 2B, right). This yielded one connection matrix per hierarchy level. We combined matrices for all hierarchy levels by piecewise multiplication of their entries (*reversing hierarchy model*, Fig. 2C1). As an alternative approach, we only considered the connection matrix for the lowest hierarchy level. Then, for each entry we considered the pair of regions it corresponds to, looked up their path distance in the hierarchy tree, and divided the value of the entry by that distance (*node distance model*, Fig. 2C2).

These models implement connectivity with a spatially continuous and distance-dependent mapping between regions that reverses at boundaries in a straight-forward manner. But they also "embed" a region hierarchy within the connectivity, once in the form of nested gradients, and once by asserting that hierarchically similar regions are more strongly connected than others. The difference between the two models is apparent already by visual inspection of their connectivity matrices (Fig. 2D).

3 Results

3.1 Testing the algorithms on the toy model

We applied the described process to the artificial model of hierarchical connectivity with depth $d = 3$ and resolution $n = 2$. We tested a *low noise* and a *high noise* condition with $\phi = 0.1$ and $\phi = 5$ respectively, i.e. a noise amplitude ten times weaker or five times stronger than the signal (Fig. 3A). In the case of the *reversing hierarchy* model (Fig. 2C1), a single application of *cosine distance clustering* or two applications of *reversal detection* resulted in a single split that aligned well with the second level of the hierarchy used (Fig. 3B1, C1). Further applications of the algorithms completely reconstructed the hierarchy under low noise conditions. When the noise level was elevated to five times the amplitude of the signal, cosine distance clustering did not recover additional

Figure 3: **Applying splitting methods on the toy model.** A: The toy models connectivity was constructed as in Fig. 2 with resolution $n = 2$ and depth $d = 3$. B1: Splitting the reversing hierarchy model using cosine distance clustering, with noise amplitudes $\phi = 0.1$ and $\phi = 5$. With low noise, a second application recovered another level of the hierarchy. B2:Splitting the node distance model using cosine distance clustering. The final hierarchy level is reached in one split with low noise. With high noise, the output is random, even after a second application. C1: Splitting the reversing hierarchy model using reversal detection. The hierarchy is almost completely recovered, but several applications are required. C2: Splitting the node distance model using reversal detection. The hierarchy is completely recovered, but the high noise condition requires a second application. D: Averaged mean gradient deviation (top) and reversal index (bottom) of the final output for the different approaches. Blue / orange: Using cosine distance clustering at low / high noise respectively. Green / red: Using reversal detection at low / high noise respectively.

Figure 4: **First split of isocortex into subregions** A1: Top: Raw values of the first five diffusion component of mouse isocortex. Bottom: Angle of the gradient at each location. A2: Left/right as A1 top/bottom for the sixth component that was selected for the split. Overlaid in black, left: Gradient field, with each vector normalized to unit length; right: Established rough parcellation (modules of Harris et al. (2019), but with MOs and SSs separated) B: Strengths of components relative to the strongest. Orange: the selected sixth components has a strength 37% of the top one. C: Lengths of vectors resulting from convolving the field in A2 with a two-dimensional Gaussian kernel with a width of five pixels. Purple outlines: Pixels with a vector length < 0.97, thus classified as a potential border. D: Resulting distance metric; drawn is the distance between any pixel and for two exemplary pixels indicated by red dots. E: Resulting first split (colored areas), with established parcellation overlaid and labelled.

granularity, and reversal detection recovered an imperfect and incomplete version. This was, because at the relatively small spatial scale, the reversing gradient was small compared to the other gradients resulting from the noise.

Conversely, for the *node distance* model (Fig. 2C2), the full parcellation was reconstructed after a single split in the low noise condition (Fig. 3B2, C2). Under the high noise condition, reversal detection required two applications, and the output of cosine distance clustering did not reflect the true parcellation in any way.

We conclude that our methods are likely to recreate at least part of a parcellation, and that resistance of the method against noise depends on the underlying architecture of connectivity, which still remains unknown. Further, the ways in which the algorithm can fail is by yielding an incomplete parcellation, or a completely incorrect parcellation. However, note that the more severe, second mode of failure was detectable through the quality metrics. Both ri and gd of the results were higher for the incorrect solution than for the correct ones. Especially ri appeared to be a good evaluator, yielding a value around two times (0.8 vs 0.4) higher in the case of the incorrect solution (Fig. 3D). For the combination of reversal detection in the reversing hierarchy model under high noise conditions, the recovered parcellation was incomplete in some parts and complete in others; this was reflected by a large standard deviation of values of ri.

3.2   Applying the algorithms to mouse cortical connectivity

We finally applied the splitting algorithm to the connectivity of the entire mouse isocortex. In all of the six strongest components, except for the first and third, a prominent reversal was immediately visible, spanning horizontally across the flat view (Fig 4A). In line with our descriptions above, we applied a first split using *reversal*

detection, which identified the sixth component as the one to use to minimize the result ri. This component had 37% of the strengths of the first, strongest component (Fig. 4B).

Closer inspection of the reversals of that component (Fig. 4A2) and comparing to an established parcellation, revealed several strong reversals. This included one starting between prefrontal and anterolateral regions (Fig. 4A2, red arrow), cutting through somatomotor regions, and ending at the point where anterolateral, somatomotor and temporal regions meet (green arrow). This led to borders being detected that surround compact regions within the somatomotor areas, as well as within temporal areas, and between medial and visual areas (Fig. 4 C). In the distance metric calculated from the result, several compact regions with low pairwise distance emerged (Fig. 4 D).

The ultimate result (Fig. 4E) led to eight subregions, where four of them covered the majority of the prefrontal, medial, anterolateral and visual modules of Harris et al. (2019) respectively. However, they also contained significant parts of the temporal module, and the somatosensory and motor areas. Consequently, the remaining four subregions covered only a small "core" of the MOs, primary somatomotor, SSs and temporal regions respectively. More formally, we calculated the intersection-over-union of the established parcellation indicated in Fig. 4E with the regions resulting from the split at reversals (Fig. 5B). We used the result to assign tentative names to the regions (Fig. 5C).

Curiously, the primary somatomotor regions were split up between six of the eight subregions detected from reversals (Fig. 4E). The apparent lack of such a fundamental level of organization as clearly delineated somatomotor regions led us to investigate more closely.

First, we found that the split of somatosensory areas between five reversal-based regions closely mirrors the split into regions associated with body parts of the established parcellation (Fig. S5A vs. B). The intersections with our anterolateral, "SSp-core" and "SSs-core" regions correspond to the mouth-, nose-, and upper limb-related parts respectively. The intersection with our visual regions corresponds to the barrel field, and medial regions to a combination of lower-limb and trunk-related parts. We conclude that reversal detection recreates the internal parcellation of somatosensory regions, but not its external borders.

Another notable result was the split of the MOs and SSs regions of the established parcellation into three subregions, located anterior, central, and posterior, respectively. We investigated the incoming and outgoing connectivities of these subregions, considering whether there is a fundamental difference in their organization, or whether they are better described as single homogeneous regions (Fig. 5A).

Unsurprisingly, each subregion interacted more strongly with its direct neighbors, but there were also fundamental differences in their long-range connectivity. While the anterior part of SSs receives its strongest inputs from anterior neighbors, the posterior part samples from medial neighbors (specifically, from the barrel field in the established parcellation). While the posterior part of MOs sends and receives extensive connectivity from prefrontal and medial areas, largely avoiding somatosensory regions, the anterior part interacts mostly with the anterior parts of primary motor and somatosensory regions. The core parts of both regions interacted mostly with each other and the core parts of primary somatosensory regions; this was mostly visible in the efferents of SSs.

Finally, the split of motor regions into subregions is arguably consistent with functional data: Guo et al. (2014) described a role of specifically the anterolateral motor areas (ALM) in an object location discrimination task that is not shared by the remaining parts of the motor regions. The ALM region aligns closely with the intersection of motor areas and the reversal-based anterolateral region.

3.3   Repeating the algorithm to create a hierarchy of regions

We continued the applications of the algorithm to detect successive splits and thereby build a hierarchy of regions. Based on our evaluation of the two algorithms, we performed a second application of *reversal detection*, as it appears to yield a more robust results, followed by three applications of *cosine distance clustering*, as it is more advantageous in smaller regions and considers more components simultaneously. In the following paragraphs we will describe the result and the reasons to stop after five applications of the algorithm.

The resulting hierarchy has 41 leaf regions at six levels (Fig. 6A1). Leaf regions exist at each hierarchy level except for the root, indicating that these regions could not be split further by the algorithm. The sizes of leaf

Figure 5: **Evaluating the first split against the established parcellation.** A: Locations of afferent (left) and efferent (right) cortical locations of regions in the established parcellation, when intersected with our parcellation. Grey lines: Established split into primary and secondary somatosensory and motor regions. White lines: Proposed parcellation of our first split. Top: Region "SSs" is split into an anterior (red stripes) core (blue dots) and posterior (green stripes) part by our parcellation. Afferent / efferent locations are indicated in red, blue and green respectively. Bottom: "MOs" is similarly split into three parts. B: Intersection over union of regions resulting from our first, reversal-based split (vertical) and the established parcellation as indicated in Fig. 4E. C: Tentative labels for the resulting regions.

regions vary considerably with the largest one being approximately eight times larger than the smallest (Fig. 6A2).

We calculated at each hierarchy level the modularity of the parcellation (see Supplementary Methods) with respect to the raw connectivity strengths and compared them to corresponding values for the established AIBS CCF hierarchy and parcellation (Fig. 5B, left). As modularity naturally decreases with increasing granularity, we plotted the results against the number of regions and compared them also to 100 random, but spatially continuous parcellations (see Supplementary Methods; Fig. 5B, black line and error bars). For both reversal-based and established schemes the modularity is significantly larger than in the random controls, but gets closer to them in the lower hierarchy levels. When we calculated modularity based on the (cosine-)similarity of connectivity instead, results were comparable (Fig. 6B, right).

Note that neither scheme aims to maximize the measure. The AIBS scheme unifies multiple historical schemes based on anatomy and neuron function, and our scheme allows very different connectivity within a subregion as long as it varies along a continuous gradient. Yet, this measure shows that our parcellation provides a qualitatively similar solution. This was also evident in a visual comparison of the connectivity matrices (Fig. S5C). Further note that to ensure comparability, we calculated modularity in the flattened view also for the AIBS parcellation; values may differ if calculated between the original voxels.

The demonstrated qualitative similarity between the reversal-based and the established solutions led to the question to what degree they actually describe the same parcellation. To quantify this, we calculated their similarity in terms of their *uncertainty coefficient*. That is, when any cortical voxel is randomly picked (but its position remains unknown), there is a large uncertainty about which of the established subregions it belongs to, which can be quantified as the *entropy* of the parcellation scheme. Once it is revealed which of the reversal-based subregions it belongs to, this uncertainty is most likely reduced, which can be quantified as a reduction in entropy (Fig. 6C, for details see Supplementary Methods). A parcellation identical to the established one would reduce the uncertainty to zero, while a parcellation largely orthogonal to it, such as the split into cortical layers, would reduce it very little. As any split into subregions is likely to reduce the entropy to some degree, we compared the results to the same

random parcellations as before. We found that the reversal-based parcellation reduced the entropy significantly *less* than the controls, i.e. it is actually more orthogonal to the established scheme than expected by chance. This indicates that differences between the schemes are due to the reversal method detecting previously unaccounted trends in connectivity and not merely generating random results or picking up noise. However, the trend weakened with number of regions until after five splits the reversal-based solution was within a single standard deviation of the controls with respect to this measurement.

As a final test, we evaluated how the reversal-based parcellation evolves with each split with respect to the previously defined quality metrics (Fig. 6 D). We found a large spread of values for both metrics, but the overall mean and median decreases reliably with each split. Occasionally, a child region results in a larger value for a metric than its parent, indicating a worse solution, but this is typically followed by an even larger decrease in the next split (Fig. 6D, inset, grey lines). Yet, after five splits, three regions were above the defined threshold for gd (Fig. 6D1, red; A2, circles), and four for ri (Fig. 6D2, red; A2, squares). All of them were above the lowest hierarchy level, indicating that the algorithm was not capable of splitting them further, and that additional applications would not lead to an improvement.

We decided to stop after five applications of the algorithm for a combination of reasons: First, at that point the parcellation was close to a random parcellation in terms of modularity and uncertainty coefficient (Fig. 6B, C). Second, the number of new regions resulting from the split had stagnated with most regions already being "atomic". Third, remaining regions with values for gd and ri exceeding the threshold could not be split by the algorithm.

4 Discussion

We have demonstrated that gradient reversals at the borders between adjacent sensory regions can also be found in the connectivity of voxels belonging to the regions. We have further demonstrated that these gradients can be isolated through the diffusion embedding technique. This approach differs conceptually from previous approaches based on clustering of matrices of connectivity similarity: While clustering-based approaches are based on the idea that connectivity profiles of voxels within a region are similar, our approach allows for dissimilar profiles, as long as the dissimilarity is the result of a continuous gradient within the region. As pointed out by Eickhoff et al. (2015), functional gradients often exist within regions (Wandell et al., 2007; Hensel et al., 2015), contradicting the underlying assumption of similarity clustering. Our method explicitly considers gradients and therefore is more likely to respect this fundamental feature of cortical architecture.

We have developed an algorithmic pipeline based on this approach that largely automatically breaks up a voxelized connectivity structure into a partition of the volume into subregions (reversal-based parcellation). In addition to the partition, the solution also provides a tentative hierarchy of subregions, although evaluations on a test model show that individual levels of the hierarchy may be swapped. At the same time, the evaluations demonstrated a very large degree of robustness against unstructured noise in the input connectivity data. We also developed quality metrics that can be used to detect algorithm failure. They can also be applied to other parcellations to evaluate how close they come to an ideal reversal-based solution.

We applied the algorithm to the voxelized connectivity of mouse isocortex. The resulting parcellation differed from established schemes, but did so in a demonstrably nonrandom way. Further, when evaluated in terms of modularity, it was further away from a random solution than the established scheme. This indicates that the reversal-based parcellation captures novel connectivity trends that cannot be detected when connectivity is evaluated with respect to the established parcellation. One example is a specialization of the anterolateral motor regions that was not present in the established parcellation, but had been described in the literature before. This demonstrates the importance of building a parcellation based on connectivity.

A feature of the established scheme that is not captured by reversal detection is the clear delineation of primary sensory areas. This can be explained by the data used: We focused exclusively on intra-cortical connectivity, while primary sensory regions are likely to be largely defined by their thalamic input sources. In the future, a parcellation could be constructed that also takes cortico-thalamo-cortical connectivity into account. Yet, even with only intra-cortical connectivity considered, our result is likely to be useful for understanding the organization of mouse cortical connectivity. In the future it may also be useful to analyze large-scale in-vivo recordings of neuronal activity with respect to our parcellation to test whether neuron function also revolves around gradient reversals in non-sensory

Figure 6: **Complete parcellation results.** A1: Tree plot of the resulting hierarchy after five successive splits (top to bottom). Size of leaf nodes proportional to region size. A2: Locations of leaf regions. Colors as in A1. Modularity of parcellations evaluated with the voxelized connectivity matrix (left) or matrix of similarity of connectivity (right). Plotted against the number of regions at each hierarchy level for the reversal-based parcellation (blue / green), a random parcellation (see Supplementary Methods) with the same number of regions (black / grey), and the AIBS CCF parcellation (red / yellow). C: Similarity of the AIBS CCF parcellation and the reversal-based parcellation, measured as their uncertainty coefficient (see Supplementary Methods). Blue bars: values at various hierarchy levels. Black dots and grey error bars: For a random parcellation with the same number of regions instead. D: Values of gd (D1) and ri (D2) indicated by the color of nodes in tree plots of the hierarchy. Red indicates values above the acceptance threshold, orange if it is an internal node. Insets: Box plots of the values after each split and the changes caused by individual splits (grey lines).

areas.

Our approach combined the reversal-based techniques with a projection into the plane defined by an area-preserving flat map, considering the resulting gradients in the plane. Mathematically, all techniques we employed could be generalized to work in three dimensions instead. *Cosine distance clustering* can be expected to work in three dimensions as well, while it remains unclear whether detected reversals would encircle subregions also in three dimensions. The quality of a solution without prior flattening can be evaluated in the future.

Our set of algorithms can be readily applied to any source of voxelized connectivity data in any organism. This includes undirected connectivity, such as functional connectomes. Additionally, data sources unrelated to connectivity can in principle be used as well, as long as a matrix of similarities between pairs of voxels can be defined and calculated. This includes for example gene expression data, although it is unclear whether this data is organized around spatial gradients with reversals.

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5 Supplementary Material

Author contributions

- Conceptualization: M.W.R.

- Data curation: M.W.R.

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Data availability

The resulting parcellation and hierarchy are available at: zenodo.org/record/7032168
And under the following DOI: 10.5281/zenodo.7032168

Supplementary Figures

Figure S1: **Framework of the diffusion embedding.** From a connectivity matrix between source voxels and target voxels, we build a similarity matrix based on how the voxels' connectivity profile is similar (A-B). On this matrix, we run the diffusion process which will strengthen high connected pathways (red) and weaken connected pathways (green) (C). This process allows to reveal an embedded geometrical space of connectivity, where strongly connected voxels are close to each and in opposite poorly connected voxels are far from each other (D). To flatten this geometrical space, we therefore extract the 2 dimensions associated with the 2 strongest eigenvectors, which we call alpha and beta components (E).

Figure S2: (A) Flattened reconstruction of the connectivity structure of the mouse isocortex by averaging the diffusion components of voxels corresponding to a pixel. (B) Standard deviation of the diffusion components of voxels corresponding to a pixel, averaged over 100 pixels.

Figure S3: **Post-processing of the initial parcellation.** Post-processing steps, as indicated in Fig. 2A, that improve the initial parcellation. A: The initial parcellation of reversal detection (top) has many unlabelled pixels (grey) in the periphery. The parcellation of cosine distance clustering (bottom) is noisy and also has unlabelled pixels. A support vector machine is trained that predicts the region label from the location of a pixel. The prediction of the SVM features straighter region boundaries and labels for all pixels. B: Occasionally, the same region label is applied to spatially non-continuous patches. For a given label, hierarchical clustering is applied to the pairwise distances of the location of associated pixels. This splits up non-continuous regions. C: The parcellation is unflattened, i.e. projected back into 3d space by looking up all voxels that are associated with a given pixel. D: Regions below a volume threshold are merged with their nearest neighbor.

Figure S4: A: Diffusion embedding performed on the whole isocortex, SSp-ll is annotated by the black line. B: Diffusion embedding of the Somatosensory and Somatomotor areas (blue and green in the parcellation in E.) C: Diffusion embedding of the Somatosensory areas (blue in the parcellation E.) D: Diffusion embedding of the SSp-ll. E: Mean gradient deviation (error bars = standard deviation) and reversal index of SSp-ll at different scales. Even though the connectivity structure of SSp-ll is homogeneous and continuous according to the gradient deviation and reversal index, it can only be revealed by isolating it after successive splits, hence the motivation to split the isocortex several time around gradients' reversals detected thanks to our method. F: Hierarchical organization of the ACCSv3.

Figure S5: A: Parcellation of primary somatatosensory regions, as defined in the established AIBS CCF. B: Intersections of primary somatosensory regions in AIBS CCF with regions at the first hierarchy level of our reversal-based parcellation. C: Matrix of connections strengths between cortical locations. C1: Rows and columns sorted by high-level regions of the established parcellation (as shown in Fig. 4E). C2: Sorted by regions in the first hierarchy level of the reversal-based parcellation. Red lines indicate breaks between regions.

5.1 Supplementary Methods

5.1.1 Diffusion embedding

The method considers a diffusion process along the edges of the graph given by the (cosine-) similarity of incoming and outgoing connectivity of each voxel. As it runs the diffusion process, pathways between nodes with dissimilar connectivity (hence weak edges in the graph) will be weaken further while strong connectivity will be strengthened. This allows the extraction of the diffusion distance between voxels, indicating their pairwise connectivity. The diffusion distance can be expressed as:

$$D_t(X_i, X_j) = \sum_{u \in X} |p_t(X_i, u) - p_t(X_j, u)|^2 = \sum_k |p_{ik}^t - p_{kj}^t|^2 \tag{10}$$

where t is the time of the diffusion process, $p_t(x, u)$ is the probability of jumping from the node x to the node u and k is the kernel defining a local measure of similarity within a certain neighbourhood. Each dimension of this coordinate system corresponds to a gradient with gradients placed in order of their strength.

5.1.2 Calculation of the uncertainty coefficient of pairs of parcellations

A parcellation X associates each voxel v with a region $r_i^X \in R^X$. We describe this association as $X(v) = i$. Let n_i^X be the number of voxels associated with r_i^X and $N^X = \sum_i n_i^X$ the total number of voxels. We can then consider P^X, the probability distribution given by the region associated with voxel that has been randomly picked (with uniform probabilities):

$$P^X : p_i^X = \frac{n_i^X}{N^X} \tag{11}$$

As with any probability distribution, we can calculate its entropy:

$$H(P^X) = -\sum_i p_i^X \cdot log(p_i^X) \tag{12}$$

Given two parcellations X, Y that are defined on the same set of voxels, we can similarly consider their joint distribution $P^{(X,Y)}$, where $p_{(i,j)}^{(X,Y)}$ is the probability that a random voxel is assigned to region i in X and to j in Y.

This allows us to calculate the mutual information of the probability distributions associated with a pair of parcellations. This is the reduction of entropy of one of them when the value of the other is revealed. That is, if you know the region identity of the random voxel according to one parcellation, how much does it help you to guess its identity in the other?

$$I(P^X; P^Y) = \sum_i \sum_j p_{(i,j)}^{(X,Y)} \cdot log\left(\frac{p_{(i,j)}^{(X,Y)}}{p_i^X \cdot p_j^Y}\right) \tag{13}$$

Normalizing it by the entropy of X yields the *uncertainty coefficient*:

$$U(P^X; P^Y) = \frac{I(P^X; P^Y)}{H(P^X)} \tag{14}$$

This is a measure of similarity between parcellations. Intuitively, if revealing that the identity of a voxel according to Y is j yields a lot of information about its its identity in X, this means there must be at least one region in X that overlaps strongly with j. Mathematically, we can see how for $X = Y$ equation 13 equals equation 12 because $p_{(i,j)}^{(X,Y)} = p_i^X = p_j^Y$ for $i = j$ and $p_{(i,j)}^{(X,Y)} = 0$ for $i \neq j$. Consequently, in that case $U(P^X; P^Y) = 1$.

Conversely, if P^X and P^Y are statistically independent, then by definition $P_{(i,j)}^{(X,Y)} = P_i^X \cdot P_j^Y$ and consequently $I(P^X; P^Y) = U(P^X; P^Y) = 0$. This is the case for orthogonal parcellations.

In the manuscript we set X to the established AIBS CCF parcellation and Y to whichever parcellation or control parcellation we want to evaluate.

5.1.3 Calculation of the modularity of a parcellation

The modularity of a parcellation with respect to a matrix of connection strengths is the difference between the fraction of connection strength that is found between pairs of voxels in the same region and the fraction of the number of pairs of voxels in the same region.

Let X be a parcellation as defined in the previous section. Let M be the connectivity matrix, such that $M(v, w)$ yields the strength of connectivity between voxels v and w. Then the fraction of connection strength found within a region is:

$$\gamma_M(X) = \frac{\sum_{v,w:X(v)=X(w)} M(v, w)}{\sum_{v,w} M(v, w)} \tag{15}$$

The fraction of voxel pairs that are in the same region, relative to all possible pairs is:

$$\phi(X) = \frac{\sum_i n_i^X \cdot n_i^X}{N^X \cdot N^X} \tag{16}$$

The modularity is then the difference between the two, $\gamma_M(X) - \phi(X)$. As individually their values are between 0 and 1. This measurement is between -1 and 1.
If connectivity strengths are independent of the parcellation, then the expected value of the measurement is 0, if strong connectivity is found predominately within a region, the measurement is > 0.

5.1.4 Generation of random control parcellations

We generated comparable, but random parcellation schemes the following way. First, a random control is paired with paired with the reversal-based parcellation after a given number of splits in order to match its number of resulting subregions. For a given number of subregions, we generated 100 random parcellations with two different algorithms (50 per algorithm).

First, we generated 50 schemes by recursively splitting the set of pixel positions of the flat view by orthogonal straight lines into two halves until the specified number of subregions is met. Each recursive iteration will double the number of subregions, thus numbers that are powers of two can be easily reached. Numbers that are not powers of two can be reached by randomly selecting a half to be split further while keeping the other intact. Different, random instances were generated by randomly selecting the angle of the line of the first split. All further splits are then along lines either parallel or orthogonal to that first line.

Second, we generated 50 schemes by first randomly distributing a number of points equal to the target number of subregions within the axis aligned bounding box of the pixel positions of the flat view. Points were randomly picked with uniform density within the bounding box. Then, pixels were classified into subregions based on the random point they were closest to.

Both controls generated random parcellations with spatially continuous subregions of various sizes and the same number of subregions as the reversal-based parcellation.