Rear cortex contraction aids in nuclear transit during confined migration by

increasing pressure in the cell posterior

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Abstract

As cells migrate through biological tissues, they must frequently squeeze through micron-sized

constrictions in the form of interstitial pores between extracellular matrix fibers and/or other cells.

Although it is now well recognized that such confined migration is limited by the nucleus, which is

the largest and stiffest organelle, it remains incompletely understood how cells apply sufficient

force to move their nucleus through small constrictions. Here, we report a novel mechanism by

which contraction of the cell rear cortex pushes the nucleus forward to mediate nuclear transit

through constrictions. Laser ablation of the rear cortex reveals that pushing forces behind the

nucleus are the result of increased intracellular pressure in the rear compartment of the cell. The

pushing forces behind the nucleus depend on accumulation of actomyosin in the rear cortex and

require Rho-kinase (ROCK) activity. Collectively, our results suggest a novel mechanism by which

cells generate elevated, intracellular pressure in the posterior compartment to facilitate nuclear

transit through 3D constrictions. This mechanism may supplement or even substitute for other

mechanisms supporting nuclear transit, ensuring robust cell migrations in confined 3D

environments.

***Key words*:** Nucleus, Confined Migration, Invasion, Cortex, Mechanobiology; Pressure

Introduction

The migration of cells through tissues is essential to many biological processes, including

embryogenesis, immune surveillance, wound healing, and cancer metastasis (Doyle et al., 2013;

Yamada and Sixt, 2019). During in vivo migration, cells must navigate through extracellular matrix

networks and layers of endothelial cells, which form constrictions as small as 1 to 2 µm in diameter

(Bone et al., 2016; Khatau et al., 2012; Weigelin et al., 2012; Wolf et al., 2013), i.e., substantially

smaller than the size of the cell and the nucleus. Although cells can readily alter their morphology

through cytoskeletal reorganization to adjust to the size of the constriction, the deformation of the

nucleus represents a unique physical challenge, as it is the largest and stiffest organelle in the

cell (Caille et al., 2002; Denais et al., 2016; Khatau et al., 2012; McGregor et al., 2016; Wolf et

al., 2013). Because of the size and stiffness of the nucleus, cells must generate substantial

intracellular forces to deform the nucleus through the constrictions. The process of deforming and

moving the nucleus through these narrow spaces, henceforth referred to as "nuclear transit," limits

the rate at which cells migrate in confined 3D environments (Davidson et al., 2015; Denais et al.,

2016; Harada et al., 2014; Jayo et al., 2016; McGregor et al., 2016; Rowat et al., 2013; Thomas

et al., 2015; Tollis et al., 2022; Wolf et al., 2013; Yadav et al., 2018).

Various mechanisms have been proposed to explain how cells accomplish nuclear transit through

confined environments (Marks and Petrie, 2022; McGregor et al., 2016). One commonly

described mechanism suggests that actomyosin and intermediate filaments at the front of the cell

pull the nucleus forward (Davidson et al., 2020; Jayo et al., 2016; Petrie et al., 2014). Other studies

have implicated pushing forces in the process, mediated through perinuclear actomyosin fibers,

which wrap around the nucleus (Thomas et al., 2015), or Arp2/3-mediated perinuclear actin

polymerization (Thiam et al. 2016). Each of these mechanisms depend on physical connections

between the nucleus and cytoskeleton. Another proposed mechanism suggests that the nucleus

is pushed forward by contraction of actomyosin in the rear cortex of migrating cells (Hetmanski et

al., 2019; Lämmermann et al., 2008; Lee et al., 2021; Mistriotis et al., 2019; Poincloux et al.,

2011). Support for pushing forces behind the nucleus derives from the observation that cells

migrating in 3D environments commonly accumulate actin in the trailing edge of the cell, and that

contraction of the cell rear often precedes nuclear transit (Hetmanski et al., 2019; Lämmermann

et al., 2008; Mistriotis et al., 2019; Thiam et al., 2016). However, functional evidence for this

mechanism is still lacking, including how forces from the contraction of the rear cortex are

transmitted to the nucleus. Lastly, many cell lines have shown the ability to migrate using multiple

modes, such as adhesion-independent "amoeboid" migration and integrin adhesion-based

"mesenchymal" migration, depending on cellular contractility and environmental adhesiveness

(Liu et al., 2015; Sahai and Marshall, 2003). This plasticity of migration modes suggests that it is

possible that cells may similarly switch between nuclear transit mechanisms in differing biological

contexts (Marks and Petrie, 2022), but experimental evidence for this has been lacking. Thus,

despite extensive previous research, several questions remain regarding the potential

mechanism cells use to apply cytoplasmic forces to the nucleus during confined migration,

including (1) how forces are transmitted from the contracting cell rear to the nucleus, and (2) to

what extent contraction of the cell rear contributes to or is necessary for nuclear transit through

small constrictions. Using microfluidic devices that mimic confined interstitial spaces, along with

advanced imaging and cellular manipulation approaches, we here report a novel mechanism by

which actomyosin in the rear cortex contracts to push the nucleus forward through constrictions.

This mechanism is associated with enrichment of actin and active myosin in the rear cell cortex

and depends on elevated RhoA-ROCK signaling. RhoA-ROCK mediated contraction of the rear

cortex results in elevated intracellular pressure in the posterior compartment of the cell, which

pushes the nucleus from behind to support migration through confined spaces.

Results

Contraction of the posterior actin cortex promotes nuclear transit through constrictions

To model cell migration through confined environments, we seeded cells into microfluidic devices

that enable the close observation of nuclear transit through precisely defined constrictions at high

spatiotemporal resolution (Davidson et al., 2015; Keys et al., 2018). In these devices, cells migrate

through collagen-coated channels with constrictions measuring 1 to 2 μm in width and 5 μm in

height (cross-sectional area ≤2×5 μm^2), formed by poly-dimethyl siloxane (PDMS) pillars

(**Fig. 1A**). The devices also feature wider control channels (15×5 μm^2) that do not require

substantial nuclear deformation during migration (**Fig. 1A**) (Davidson et al., 2015). The size of the

narrow constrictions reflects the geometries of small pore sizes that migrating cancer cells

encounter in vivo (Weigelin et al., 2012), while the width of the control channels was chosen to

be wider than the typical diameter of nuclei (Lammerding, 2011) and corresponds to the upper

range of interstitial spaces (Weigelin et al., 2012). We have previously demonstrated that the

5 μm height is sufficient to vertically confine migrating cells, and that cells adhere to both top and

bottom surfaces of the cell, plus the vertical walls (Davidson et al., 2015, 2014), thereby creating

true 3D confined environments that model confined migration *in vivo* (Denais et al., 2016; Wang

et al., 2022). These devices provide several advantages over imaging cells migrating through

collagen matrices, as they enable long-term imaging of cells migrating along a single focal plane,

through precisely defined constriction geometries. In contrast, in vitro assembled collagen

matrices have heterogeneous, randomly distributed constriction geometries and often lead to cells

migrating out of the imaging plane during prolonged image acquisition series.

Figure 1. Cortex-driven nuclear transit provides an advantage to cells migrating through narrow

constrictions. (**A**) Schematic layout of microfluidic device used to study confined migration through

precisely defined constrictions. (i) Reservoirs for cell media; (ii) seeding ports to add cells; (iii) seeding area

where cells attach prior to migration through constrictions; (iv) constriction area, shown in detail in inset, to

the right. The inset shows areas with constrictions (left) and the larger control channels (right), with the

corresponding cross-sections listed below each area. (**B**) Representative image sequences of MDA-MB-

231 cells co-expressing fluorescently labeled histones (mNeonGreen-H2B, cyan) and actin (mCherry2-

actin chromobody, magenta). MDA-MB-231 cells adopt varying morphological characteristics as the

nucleus squeezes through microfluidic constrictions using either (i) a rear cortex-driven mechanism, or (ii)

a non-cortex driven mechanism. Scale bar: 20 µm. (**C**) Relative frequency of cortex-driven and nuclear

transit mechanisms in varying cell types migrating through either narrow constrictions (≤2×5 µm^2) or wider

control channels (15×5 µm^2). Error bars represent 95% confidence intervals. ****, *p < 0.0001*, based on a

Chi-Squared test of independence. Circles represent means of experimental replicates. (**D**) Nuclear transit

times through ≤2×5 µm^2 constrictions of different cell types, subdivided into cortex-driven and non-cortex

driven nuclear transit mechanisms. Red line represents sample mean. Error bars represent standard

deviation. **, $p < 0.01$; ****, $p < 0.0001$, based on one-way ANOVA.

We chose to study MDA-MB-231 metastatic breast cancer cells because they exhibit the ability

to switch between different migration modes (Geiger et al., 2019; Sahai and Marshall, 2003) and

therefore may use multiple mechanisms to drive nuclear transit. MDA-MB-231 cells stably

expressing fluorescently labeled histones (mNeonGreen-H2B Histone (Davidson et al. 2015)) and

actin (mCherry2-actin chromobody (Chromotek)) exhibited two distinct patterns of actin

accumulation around the nucleus while migrating through constrictions in microfluidic migration

devices. Most cells formed a rounded, actin-enriched cortex in the rear of the cell, the contraction

of which was associated with the nucleus squeezing through the constriction (**Fig. 1B-i, Supp.**

Movie 1). In other cells, the nucleus transited through the constriction without the cell forming a

rounded rear cortex (**Fig. 1B-ii**). Notably, whereas the formation of a distinct, rounded rear cortex

was observed in the majority of MDA-MB-231 cells migrating through narrow constrictions, it was

rarely observed in cells migrating through the larger control channels, nor in cells migrating on 2D

glass substrates (**Fig. 1B-iii, 1C, Supp. Fig. S1C**). We observed similar patterns of actin

accumulation at the rear of MDA-MB-231 cells migrating through 3-dimensional collagen matrices

(**Supp. Fig. S1**). Together with previous observations of the formation of a rounded rear cortex in

MDA-MB-231 cells during transendothelial migration (Chen et al. 2016), our results indicate that

these nuclear transit mechanisms are relevant during migration in physiological environments.

We hypothesized that the differences in cytoskeletal organization prior to and during nuclear

transit indicate two distinct nuclear transit mechanisms, which may correspond with the previously

described "pushing" and "pulling" forces. Accumulation of actin in the rear cortex suggests a

"cortex-driven" pushing of the nucleus from behind, whereas accumulation of actin in front of the

nucleus suggests "non-cortex-driven" pulling at the front of the nucleus. We recorded similar actin

dynamics in HT1080 fibrosarcoma cells in microfluidic migration devices (**Fig. 1C, Supp. Fig.**

S2B), another cancer cell line that shows considerable plasticity in its migratory mode (Petrie et

al., 2016; Wolf et al., 2003). In contrast, mouse embryonic fibroblasts (MEFs), which tend to use

a mesenchymal migration mode (Gadea et al., 2007), predominantly used a non-cortex driven

nuclear transit mode (**Fig. 1C, Supp. Fig. S2A, Supp. Movie 2**).

Based on these observations, we hypothesized that the rear cortex contraction may aid MDA-

MB-231 and HT1080 cells in nuclear transit through narrow constrictions by applying "pushing"

forces to the nucleus from the back of the cell. To determine whether the rear cortex contraction

produced more rapid nuclear transit, we compared the transit times between cells using either

(rear) cortex-driven or non-cortex driven nuclear transit for each of the cell lines. In MDA-MB-231

and HT1080 cells, cortex-driven cells translocated their nuclei significantly faster through narrow

constrictions than non-cortex-driven cells (**Fig. 1D**), suggesting that in these cell types, the rear

cortex contractions provide an advantage over non-cortex driven migration. In contrast, we did

not find any differences in nuclear transit time in in MEFs using either the cortex or non-cortex

driven mechanism (**Fig. 1D**). The preference towards a cortex-driven mechanism seen in MDA-

MB-231 and HT1080 cells, in contrast to MEFs, may be due to the greater migratory plasticity

that is commonly observed in these cancer cell lines (Sahai and Marshall, 2003). As MDA-MB-

231 and HT1080 cells are capable of migrating using both mesenchymal and amoeboid migration

modes, depending on environmental and biological factors, they may be able to use this additional

cortex-driven nuclear transit mechanism to support passage through narrow constrictions. MEFs,

in contrast, are more conventionally mesenchymal in their migration (Gadea et al. 2007), and

therefore may be less able to use this additional migration mechanism. Taken together, these

results suggest that rear cortex contraction may act as an alternative or supplemental mechanism

in confined migration, which enables more rapid migration through constrictions but is not

necessarily required for nuclear transit.

Since previous studies had suggested that pulling forces at the leading edge of the nucleus

require connections between the nucleus and cytoskeleton (Petrie et al. 2014, Davidson et al.

2021), we investigated whether disruption of the linker of nucleoskeleton and cytoskeleton (LINC)

complex caused a switch to a cortex-driven nuclear transit mechanism. MEFs expressing GFP-

Nesprin-2 (Davidson et al. 2021) and mCherry2-Actin chromobody were transfected with a BFP-

tagged dominant-negative KASH construct (DN-KASH), which binds with Sun proteins at the

nuclear envelope and prevents the association between Sun proteins and endogenous Nesprin

proteins, thereby disrupting force transmission between the cytoskeleton and nucleus (Lombardi

et al. 2011). Whereas GFP-Nesprin-2 was localized to the nuclear envelope in non-modified cells

and in cells expressing a BFP-only control constructs, in DN-KASH expressing MEF cells,

Nesprin-2 was mislocalized from the nuclear envelope to the ER (**Supp. Fig. S3A & B)**, confirming

disruption of the LINC complex by the DN KASH construct. Surprisingly, LINC complex disruption

did not correspond with increased nuclear transit times, nor in a shift towards a cortex-driven

mechanism (**Supp. Fig. S3C & D**). These findings suggest that nuclear transit can be

accomplished in the absence of the LINC complex, and neither cortex-driven nor non-cortex

driven nuclear transit mechanisms require an intact LINC complex.

Pushing forces behind the nucleus are generated by actomyosin contraction in the rear

cortex

We hypothesized that cortex-driven cells localize contractile machinery to the rear cortex to push

the nucleus through constrictions. Previous studies found that non-muscle myosin II is important

for force generation during 3D confined migration (Davidson et al. 2020; Thomas et al. 2015);

thus, we performed time lapse video microscopy on MDA-MB-231 cells transfected to transiently

express GFP-myosin IIA and mCherry-myosin IIB in the migration devices. Both myosin II

isoforms localized to the rear cortex of cells as the nucleus squeezed through constrictions

(**Fig. 2A**). Notably, the accumulation of myosin II at the rear cortex was only observed in cells

migrating through narrow constrictions, whereas in cells migrating through larger control channels

or on 2D surfaces, i.e., in situations not utilizing rear-cortex driven nuclear transit, myosin II was

localized to the front of the cell body or the leading edge of the nucleus (**Fig. 2A, Supp. Fig. S4A-**

B). Importantly, our studies also revealed that individual cells can switch between non-cortex-

driven and cortex-driven mechanisms during nuclear transit. In some instances, cells that entered

constrictions with GFP-myosin II initially primarily localized at the leading edge of the nucleus

failed to pass through constrictions. When the nuclear transit attempt was not successful, the cells

backed out of the constriction, and re-entered the constriction with GFP-myosin IIA localized to

the rear cortex, using rear cortex contraction to successfully push the nucleus through the

constriction (**Supp. Movie 3**). These findings suggest that cells may actively switch between

nuclear transit modes while squeezing through small constrictions.

To map myosin activity, rather than observe only the distribution of myosin, we

immunofluorescently labeled cells fixed inside the microfluidic devices for phosphorylated myosin

light chain (pMLC), an indicator of active actomyosin contractility. Cells in which the nucleus had

just begun to enter the narrow constrictions displayed characteristic pMLC localization at the rear

cortex of cells, indicating that the rear cortex actively contracts with the onset of nuclear transit

(**Supp. Fig. S4C**). Importantly, the localization of pMLC to the rear cortex was only observed in

cells undergoing nuclear transit through narrow constrictions, and was not seen in cells migrating

through wider control channels or on 2D substrates, consistent with our prior observations that

cells only use the cortex-driven mechanism when encountering small constrictions (**Supp. Fig.**

S4C). Of note, pMLC was also found at the leading edge of the nucleus, suggesting that cortex-

driven cells may also apply complementary pulling forces at the leading edge of the nucleus or

that myosin II activity is required for the protrusion and extension of the leading edge (**Supp. Fig.**

S4C).

Figure 2: Rear cortex driven nuclear transit is associated with localization of myosin II to the rear cortex. (**A**) Representative time-lapse series of MDA-MB-231 cells expressing GFP-myosin IIA and mCherry-myosin IIB migrating through microfluidic migration devices. White arrows indicate accumulation of myosin II at the rear cortex. Magenta arrows point to accumulation in front of the nucleus. The nucleus is outlined in yellow for better visibility in the merged image. Scale bars: 20 µm (**B**) Percentage of nuclear transit events using cortex-driven or non-cortex driven modes in either ≤2×5µm^2 or 15×5µm^2 constrictions

following treatment with either RhoA activators (RhoActII or LPA), ROCK inhibitor (Y27632), or vehicle

control. Error bars represent 95% confidence intervals. **, $p < 0.01$; ****, $p < 0.0001$, based on a Chi-

Squared Test of Independence. Circles represent mean of each experimental replicate. (**C**) Nuclear transit

times of MDA-MB-231 cells migrating through constrictions following treatment with RhoA activators

(RhoActII or LPA) or ROCK inhibitor (Y27632). Red line represents mean. Error bars represent standard

deviation. **, $p < 0.01$; ***, $p < 0.001$; ****, $p < 0.0001$, based on a one-way ANOVA. Number of cells in

each group indicated below the graphs.

Since myosin contractility is regulated through RhoA and Rho-associated protein kinase (ROCK)

(Ridley 2003), we hypothesized that cells locally activate RhoA in the rear cortex to generate

actomyosin contractile forces to push the nucleus from behind. To record the spatiotemporal

dynamics of RhoA activation during nuclear transit, we stably modified MDA-MB-231 cells with a

previously established FRET-based biosensor for RhoA activity (Pertz et al. 2006) and imaged

the cells as they migrated through constrictions. Local RhoA activity was determined by

measuring the average FRET ratio in either the rear cortex, front cortex, or directly in front of the

nucleus (**Supp. Fig. S5A**). Since levels of the RhoA sensor inside the nucleus were very low, as

expected, which could negatively affect the robustness of ratiometric FRET analysis, the nucleus

was masked-out and excluded from the analysis (**Supp. Fig. S5A**). FRET ratios of the RhoA

biosensor were evaluated prior to nuclear transit ("Pre"), during nuclear entry into a constriction

("Entry"), immediately upon nuclear exit from the constriction ("Exit"), and after the cell had left

the constriction ("Post") (**Fig. 3A**). In cells migrating through narrow constrictions, RhoA activity

was elevated in the rear cortex relative to the rest of the cell body throughout nuclear transit

(**Fig. 3B**). Of note, increased RhoA activity in the rear cortex was unique to cells migrating through

narrow 3D constrictions and was not observed in cells migrating through the wider control

channels or on 2D substrates (**Supp. Fig. S5B**). In confined conditions, RhoA activity in the rear

cortex increased as the nucleus entered the constriction, and then returned to baseline levels

during the later stages of nuclear transit (**Fig. 3C**). Unlike RhoA activity at the rear cortex, RhoA

activity in the front cortex remained constant throughout nuclear transit (**Supp. Fig. S5D**). RhoA

activity in front of the nucleus (**Supp. Fig. S5A, yellow zone**) did not increase upon nuclear entry

into the constriction but increased at the end of nuclear transit (**Supp. Fig. S5C**). Collectively,

these observations suggest a sequential process in which RhoA is first activated at the posterior

of the cell, causing contraction of actomyosin in the rear cortex to push the nucleus into a

constriction, followed by activation of RhoA in front of the nucleus to contract actomyosin at the

leading edge of the nucleus to pull the nucleus through the constriction.

Figure 3. Cortex-driven nuclear transit is associated with increased RhoA activity at the rear cortex.

(**A**) Representative time lapse series of FRET ratio of MDA-MB-231 cell expressing RhoA-FRET biosensor

migrating through a microfluidic constriction. The bottom series shows the RhoA-FRET ratio during nuclear

transit, illustrating increased RhoA activity at the rear cortex (arrow) and the leading edge of the cell. Scale

bars: 20 µm (**B**) Comparison of RhoA activity at different intracellular locations based on the recorded RhoA-

FRET values for cells migrating through ≤2×5 µm² constrictions. Each data point represents local RhoA

FRET measurements averaged across all time points during a single nuclear transit event. Black lines

represent the mean for each group. **, $p < 0.01$ using paired non-parametric Wilcoxon test. (**C**) Time course

of FRET ratio within rear cortex of individual cells (normalized to average FRET ratio of whole cell) at each

phase of nuclear transit through ≤2×5µm² constrictions. *, $p < 0.05$ using paired non-parametric Wilcoxon

test.

As the cortex-driven nuclear transit mechanism was associated with active RhoA and myosin II

at the rear cortex, we hypothesized that the cortex-driven nuclear transit mechanism would

depend on Rho-ROCK activity. We treated cells with either ROCK inhibitor (Y27632) or RhoA

activators (LPA or RhoA Activator II) and measured nuclear transit times in the microfluidic

devices. ROCK inhibitor treatment significantly slowed nuclear transit through the constrictions

but did not slow migration through unconfined channels (**Fig. 2C**), suggesting that ROCK activity

is particularly important for confined migration. Interestingly, ROCK inhibition increased the

frequency of non-cortex driven nuclear transit events and altered localization of myosin IIA and

IIB during nuclear transit, causing myosin to localize towards the front of the nucleus, rather than

in the rear cortex as is seen in vehicle control cells (**Fig. 2A-B**). As ROCK inhibition slowed down

nuclear transit through narrow constrictions but not through unconfined channels, this also

suggests that the role of ROCK in pushing the nucleus from behind is unique to nuclear transit

through narrow constrictions. This mirrors our earlier observation that cells in unconfined channels

rarely use a cortex-driven migration mode. Ectopic activation of RhoA with either LPA or RhoA

Activator II had no effect on the nuclear transit rate or nuclear transit mechanism in MDA-MB-231

cells (**Fig. 2C**). The lack of effect of pharmacological RhoA activators on nuclear transit rate or

mechanism may indicate that RhoA in these cells was already highly activated by FBS in the cell

media, or that global RhoA activation without spatial control within the cell is insufficient to activate

the cortex-driven transit mechanism. Although actomyosin contractility likely plays a role in both

cortex-driven and non-cortex driven mechanisms, these results further suggest that cortex-driven

nuclear transit requires a particularly high level of Rho-ROCK mediated contractility in contrast to

non-cortex driven nuclear transit.

Laser ablation of the cell cortex reveals a pressure-driven nuclear transit mechanism

Having established that cortex-driven cells localize actomyosin and active RhoA to the rear cortex

at the beginning of nuclear transit, we hypothesized that contraction of the rear cortex pressurizes

the rear compartment of the cell relative to the front compartment, pushing the nucleus forward

through the constriction. To probe differences in intracellular pressure generated by rear cortex

contraction, we used a two-photon laser to ablate specific cytoskeletal regions of migrating cells

while they squeezed their nucleus through microfluidic constrictions (**Fig. 4A).** As the nucleus

transits through a constriction, the cytoskeletal forces pushing or pulling on the nucleus are

counteracted by the resistance of the constriction in the form of the friction and the normal forces

at the interface between the nucleus and the constriction (**Supp. Fig. S6B-C**).

Targets for laser ablation were selected based on previously hypothesized roles in applying

pushing or pulling forces on the nucleus during nuclear transit, including: (i) perinuclear actin

filaments at the leading edge of the nucleus ("Nuclear Front"), which pull the nucleus forward, (ii)

the rear cortex, whose contraction pushes the nucleus from behind ("Rear"), (iii) the front cortex

at the leading edge of the cell, which may retain pressure in the front compartment of the cell that

could inhibit nuclear transit ("Front"), (iv) both cortexes simultaneously to compare

compartmentalized pressure in the front and rear of the cell body ("Both"), and (v) non-ablated

cells to control for spontaneous movement of the nucleus during experiments (**Fig. 4A**). If

contraction of the rear cortex pushes the nucleus forward, then ablation of the rear cortex during

nuclear transit is expected to result in the nucleus falling backwards (**Supp. Fig. S6C**). On the

other hand, if the nucleus is pulled forward by actomyosin fibers at the leading edge of the

nucleus, as has been previously shown in MEFs (Davidson et al. 2020), then ablation at the

nuclear front should result in the nucleus moving backwards (**Supp. Fig. 6C**). In contrast, ablation

of the front cortex, which may inhibit forward movement of the nucleus through maintaining

increased pressure in the front compartment of the cell (Petrie et al. 2014), is expected to result

in forward movement of the nucleus (**Supp. Fig. S6C**). In all cases, movement of the nucleus in

response to laser ablation is expected to occur almost instantaneously, as ablation should

immediately disrupt the balance of forces acting on the nucleus, and nuclear movement will only

be resisted by viscous forces within the cytoplasm (in the case of rearward movement) or the

resistance of microfluidic constrictions (in the case of forward movement).

As seen in previous studies (Charras et al. 2005; Mistriotis et al. 2019; Tinevez et al. 2009),

ablation of the cell cortex caused the formation of a large plasma membrane bleb, indicating the

release of cytosolic pressure (**Fig. 4B, Arrow**). Ablation of the rear cortex and formation of the

bleb at the cell posterior led to transient rearward movement of the cell nucleus (**Fig. 4B-D**). This

observation supports our hypothesis that contraction of the rear cortex pushes the nucleus from

behind by increasing intracellular pressure in the rear compartment. Furthermore, recovery and

contraction of the bleb within a minute of the initial laser ablation resulted in forward movement of

the nucleus (**Fig. 4B-D**), indicating that restoration of the cell rear cortex increased intracellular

pressure in the back of the cell and pushed the nucleus forward.

Following ablation of the front cortex of cells, the nucleus moved forwards, suggesting that prior

to ablation, pressure in the front compartment of the cell impeded forward movement of the

nucleus (**Fig. 4C-D, Supp. Fig. S6A**). However, the magnitude of the nuclear forward movement

was less than the rearward movement observed when ablating the rear cortex, suggesting that

pressure in the rear compartment may be greater than the pressure in the front compartment

(**Fig. 4C-D**). To directly assess whether the pressure is greater in the rear compartment of the

cell than in the front compartment, we ablated both front and rear cortexes of the cell

simultaneously **Fig. 4C-D**). Ablation of both cortexes led to a rearward shift of the nucleus,

confirming that the pushing force generated by the pressure from the rear cortex contraction was

greater than the resisting force generated by pressure from the front compartment (**Fig. 4C-D**).

Figure 4. Nuclear movement following laser ablation of local actin cytoskeleton reveals that cortex-

driven nuclear transit results from increased pressure in the rear compartment. (**A**) Laser ablation

set-up. Dashed boxes represent regions targeted for laser ablation in cells starting to undergo nuclear

transit through a small (≤2×5 μm^2) constriction. Cells were modified to stably express mNeonGreen-H2B

and mCherry actin-chromobody to visualize nuclear movement and actin cytoskeleton, respectively. (**B**)

Representative time lapse series of cell ablated at the rear cortex. Yellow box represents laser ablation

target. Arrow shows plasma membrane bleb formation post-ablation. Dashed green box corresponds with

inlay of mNeonGreen-H2B Histone signal on right. In inlay region: dashed white line represents starting

point of leading edge of nucleus. (**C**) Trace of nuclear centroid shift following laser ablation. Error bars

represents mean ± SEM, based on 13-16 cells per condition. (**D**) Quantification of peak nuclear centroid

shift immediately following nuclear ablation. Red line represents mean, black error bars represent standard

deviation. *, $p < 0.05$; **, $p < 0.01$ based on unpaired non-parametric Kruskal Wallis test. (**E**) Cross-sectional

area of blebs formed after cortex ablation. *, $p < 0.05$ for paired non-parametric Wilcoxon test; ****, $p <$

0.0001 based on unpaired non-parametric Kruskal-Wallis test. Cell counts per condition shown below

graph. Red lines represent mean, black error bars represent standard deviation.

As an additional means of comparing pressure between the front and rear compartments of the

cell, we measured the size of blebs in the cell cortex formed as a result of cortex ablation (**Fig. 4E**).

Previous work had demonstrated that bleb size following laser ablation increases as a

consequence of elevated intracellular pressure, and is limited only by the elasticity of the cell

membrane (Tinevez et al. 2009). Thus, increased bleb sizes following laser ablation indicate

increased intracellular pressure prior to ablation. Following simultaneous ablation of the front and

rear cortexes, blebs formed in the rear compartment were significantly larger than blebs in the

front compartment, indicating that pressure in the rear of the cell is greater than pressure in the

front compartment (**Fig. 4E**). Collectively, these findings confirm that increased pressure at the

cell rear helps to push the nucleus forward through constrictions.

Ablation directly in front of the nucleus led to a subtle rearward shift of the nucleus, suggesting

the presence of pulling forces at the leading edge of the nucleus (**Fig. 4 B-C, Supp. Fig. S6A**),

consistent with previous findings (Davidson et al. 2020). However, the rearward movement of the

nucleus was very modest in comparison to the movement following rear cortex ablation (**Fig. 4D**).

These findings indicate that the cortex-driven cells may rely more heavily on pushing forces from

behind the nucleus, than on pulling forces at the nuclear front, which is also consistent with the

faster nuclear transit we observed in the cells using the cortex-driven mechanism (**Fig. 1D**).

We hypothesized that these intracellular pressure-driven pushing forces resulted from the

accumulation and contraction of actomyosin in the rear cortex during cortex-driven nuclear transit.

As we observed that ROCK-inhibition reduced myosin accumulation in the rear cortex, we

hypothesized that ROCK inhibition would reduce intracellular pressure behind the nucleus.

Following Y27632 treatment, nuclear movement following rear cortex ablation was reduced,

whereas nuclear shift in response to ablation of the nuclear front was unaffected (**Fig. 4D**),

indicating that pushing forces between the rear cortex and nucleus result from ROCK-dependent

actomyosin contractility. Additionally, ROCK inhibition led to a substantial decrease in the size of

blebs formed following laser ablation (**Fig. 4E**), further confirming that ROCK mediated

actomyosin contractility drives contraction of the rear cortex and increased cytosolic pressure in

the rear compartment of the cell.

Discussion

In this study, we investigated the cytoskeletal dynamics and intracellular forces acting on the

nucleus as cells migrate through confined spaces. We identified a novel mechanism by which

contraction of actomyosin at the rear cortex pushes the nucleus through constrictions during 3D

migration. Our results suggest that cortex-driven nuclear transit is a distinct mechanism from

alternative "non-cortex-driven" mechanisms, which have been described previously (Davidson et

al. 2020; Petrie et al. 2014). In the cortex-driven nuclear transit mechanism, pushing forces at the

cell rear are generated through contraction of actomyosin in the posterior cortex, which elevates

cytosolic pressure behind the nucleus to push the nucleus forwards (**Fig. 5**). This contrasts the

"non-cortex-driven" modes, in which pulling forces, through actomyosin or intermediate filaments,

are mediated through physical connections between the nucleus and cytoskeleton (Davidson et

al., 2020; Petrie et al., 2014; Thomas et al., 2015) (**Fig. 5**). Our studies suggest that some cell

lines are able to use both mechanisms to achieve nuclear transit, though individual cell lines may

have a propensity to use one mechanism over another. It remains to be elucidated whether these

pushing and pulling mechanisms work independently to accomplish nuclear transit, or whether

they act complimentarily.

Figure 5: Model of alternate mechanisms of nuclear transit through constrictions. Pushing forces are

generated through contraction of the posterior cortex, caused by co-localization of active RhoA, Myosin II,

and Actin. Co-localization of these same proteins at the leading edge of the nucleus can generate pulling

forces at the front of the nucleus, mediated through the LINC complex.

Mirroring our findings in microfluidic devices and collagen matrices, accumulation of actomyosin

in the rear of cells migrating in 3D has been observed in MDA-MB-231 cells invading through

Matrigel (Poincloux et al., 2011) and in vitro models of transendothelial migration (Chen et al.

2016), indicating that cortex-driven nuclear transit may play an important role in these

physiological processes. Earlier studies of 3D dendritic cell migration reported that retraction of

the cell rear preceded nuclear squeezing through constrictions (Lämmermann et al., 2008). These

studies showed that inhibition of contractility through treatment with blebbistatin and Y27632

delayed contraction of the cell posterior, which corresponded with a reduced migration rate in

confined environments (Lämmermann et al., 2008; Schaar and McConnell, 2005). However, it

was unclear whether this retraction represented a direct transmission of force between the rear

cortex and the nucleus, or whether rear retraction followed the forward movement of the nucleus.

More recent findings have found elevated RhoA activity and myosin at the rear of cells migrating

through 3D channels and showed evidence that this resulted in increased intracellular pressure

behind the nucleus (Mistriotis et al., 2019). However, these studies did not address how

intracellular pressure could contribute to nuclear transit through constrictions. Our results build

upon these prior findings by confirming that retraction of the rear cortex pushes the nucleus

forward during nuclear transit, and by demonstrating a functional role for cortex-driven pressure

generation in confined 3D migration.

Our findings complement prior studies which have probed intracellular forces acting on the

nucleus during cell migration. One such set of studies evaluated the role of pulling forces at the

front of the nucleus, which increase intracellular pressure in the front compartment of fibroblasts

and HT1080 cells migrating through 3D environments (Petrie et al., 2016, 2014). In contrast with

our work, these studies used a probe to directly measure intracellular pressure in cells migrating

through 3D cell-derived matrix. They found that actomyosin and intermediate filaments at the

nuclear front pulled the nucleus forward to increase pressure at the leading edge of cells, which

generated "lobopodia" to enable invasion through 3D environments. However, subsequent

studies in mesenchymal stem cells migrating in 3D alginate hydrogels have indicated that pulling

forces at the leading edge of the nucleus are not necessary for the formation of lobopodia (Lee et

al., 2021). In the absence of nesprins, the nucleus was still able to move forward into constrictions

to pressurize the front compartment of cells, while the authors noted an accumulation of pMLC in

the rear cortex. These results mirror our findings of active RhoA and pMLC in the rear cortex

during nuclear entry to constrictions, supporting the idea that elevated pressure at the cell rear is

increased at the beginning of nuclear transit.

One limitation of our studies is that our detection of intracellular forces must be inferred from

protein localization and changes in nuclear position following laser ablation, rather than measuring

these forces directly, as the PDMS enclosure of the microfluidic migration devices prevents direct

access to the migrating cells. Our laser ablation assay is limited as an indirect measurement of

intracellular pressure (or other cytoskeletal forces), as it only reveals forces acting on the nucleus

at a single point in time, though the pressure throughout the cell body during nuclear transit may

be highly dynamic as the nucleus shifts from the rear compartment of the cell to the front

compartment. Additionally, the laser ablation likely disrupts not only actomyosin but also other

force-generating cytoskeletal structures within the target region, including intermediate filaments

and microtubules, which could further contribute to the force transmission and force generation.

Nonetheless, as we found that the cortex-driven mechanism strongly depends on the Rho-ROCK-

myosin pathway, we believe that this mechanism principally depends on actomyosin activity,

though our results cannot rule out potential contributions of other cytoskeletal elements, which

have previously been implicated in nuclear movement (Petrie et al., 2014; Tsai et al., 2010). In

addition, the distinct circular shape of rear cortex, in contrast with that of front cortex, further

supports the conclusion that the pressure is higher in the rear compartment.

A recent report demonstrated the role of pulling forces in mediating nuclear transit in MEFs

(Davidson et al., 2020). Similar to our results in MDA-MB-231 cells, the authors demonstrated

that ROCK inhibition increases nuclear transit times of MEFs migrating through narrow

constrictions, but not through unconfined 3D channels (Davidson et al., 2020). Using a laser

ablation assay, as we have used here, they found that ablation in front of the nucleus caused a

rearward shift in the nucleus whereas ablation at the cell rear had no effect on nuclear movement.

They also found that the rearward shift in nuclear position following ablation at the nuclear front

was dependent on connections between the nucleus and cytoskeleton. These results contrast

with our own using MDA-MB-231 cells, as we detected only very subtle nuclear shifts following

ablation of the nuclear front, a significant rearward shift of the nucleus after rear cortex ablation,

and LINC complex disruption did not impede nuclear transit (**Supp. Fig. S3**). This difference in

results could be attributable to our findings that MEFs scarcely use the cortex-driven nuclear

transit mechanism in comparison to MDA-MB-231s, which very frequently used the cortex-driven

mode. These two findings are complementary in that they highlight a key difference between

MEFs, which in the "non-cortex-driven" mode apply pulling forces at the front of the nucleus

(Davidson et al., 2020), and cortex-driven MDA-MB-231 cells which push the nucleus from behind

through intracellular pressure generated by the rear cortex.

Although we have noted a cell-type specific preference towards the cortex-driven mechanism,

and that the mechanism depends on high Rho-ROCK-mediated contractility, it remains unclear

what biological or environmental factors cause individual cells to adopt a particular nuclear transit

mechanism. As others have found that pulling forces at the front of the nucleus depend on the

LINC complex (Davidson et al., 2014; Petrie et al., 2016), it is possible that the cortex-driven

mechanism could compensate for a lack of pulling forces in specific scenarios. For example,

pulling forces at the leading edge of the cell require adhesions to the surrounding environment.

Thus, cells that migrate in an adhesion-independent "amoeboid" migration mode may require

cortex-driven forces for nuclear transit through narrow constrictions, or cells may benefit from an

additional 'boost' from the cortex-driven pressure when pulling forces are insufficient to move the

nucleus through a constriction. Surprisingly, in our studies using a dominant negative nesprin

construct (DN KASH), we found that LINC complex disruption did not alter nuclear transit time nor

nuclear transit mode. Future studies will be necessary to determine the specific factors

determining the selection of a particular migration mechanism, and whether this is an active

decision-making process requiring specific signaling pathways, or whether cells use multiple

migration modes in parallel, with a specific mode dominating depending on the particular

microenvironment (Liu et al., 2015; Wolf et al., 2013; Friedl and Wolf, 2010; Geum et al., 2016).

In discovering this novel mechanism for cortex-driven nuclear transit, we have opened a number

of prospective avenues that will improve the understanding of how cells traverse confining 3D

environments. An improved understanding of the diverse mechanisms cells have available to

overcome narrow interstitial spaces and how cells select between these mechanisms may lead

to new targets for therapies to reduce or prevent cancer cell invasion and metastasis, or to boost

the migration of immune cells to sites of infection.

Methods

Cell Culture

MDA-MB-231 metastatic breast adenocarcinoma cells were purchased from American Type

Culture Collection (ATCC); HT1080 fibrosarcoma cells were a gift from Peter Friedl and Katarina

Wolf, originally purchased from DSMZ in Braunschweig, Germany; MEFs expressing GFP-

Nesprin-2 were a gift from Cecile Sykes; MDA-MB-231 cells expressing the RhoA-FRET

biosensor were a gift from Louis Hodgson. All cell lines were cultured in Dulbecco's Modified

Eagle Medium (DMEM) supplemented with 10% (v/v) fetal bovine serum (FBS, Seradigm VWR),

and penicillin and streptomycin (50 U/mL, ThermoFisher Scientific) and were maintained at 37°C

and 5% CO_2. Cell lines were modified to express fluorescently tagged proteins using lentiviral

vectors (pCDH-mCherry2-Actin Chromobody-puro and pCDH-mNeonGreen-H2B Histone-puro).

Transient expression of CMV-GFP-NMHC-IIA (Addgene #11347) and mCherry-MyosinIIB-N-18

(Addgene #55107) was achieved using a Nucleofector II electroporator and the Cell Line

Nucleofector Kit V (Lonza Biosciences). MEF were modified using BFP and DN-KASH expression

plasmids in a doxycycline-inducible Piggybac plasmid backbone (Addgene #187019). Cell lines

were tested for mycoplasma infection following completion of experiments. Human cell lines were

verified through the ATCC Cell Line Authentication Service.

Viral and Piggybac Modification

Pseudoviral particles were produced using 293TN cells (System Biosciences, SBI) were

transfected with the lentiviral plasmid of interest as well as lentiviral packaging and envelope

plasmids (psPAX and pMD2.G, gifts from Didier Trono) using PureFection transfection reagent

(SBI), per manufacturer's protocol. Supernatants were collected at 48, 72, and 96 hour intervals

post-transfection and were passed through a 0.45 μm filter. Cells to be transduced were cultured

for 24 hours prior to transduction at a confluency of 50% and were then cultured in lentivirus-

containing media with polybrene (8 μg/mL). Lentivirus containing media was removed after 24

hours, and following an additional 24 hours of recovery time, cells were selected using 1 μg/mL

of puromycin (Invivogen) for 3 days. For Piggybac modifications, MEFs were seeded into 6-well

plates and were transfected with 1.75 μg of Piggybac plasmids and 0.75 μg of a hyperactive

transposase using PureFection Transfection reagent (SBI), per manufacturer's protocol.

Transfected cells were selected using 800 μg/mL G418 for 3 days. Cells were sorted using flow

assisted cell sorting (FACS) in order to obtain consistent expression levels.

Microfluidic Device Preparation

Microfluidic devices were prepared as previously described (Davidson et al., 2015; Keys et al.,

2018). Briefly, microfluidic devices were made through soft lithography by curing

polydimethylsiloxane (PDMS) in a plastic mold containing microfluidic features at 65°C for 2

hours. After removing cured PDMS from the mold, PDMS features were cut out using biopsy

punches, and then both PDMS devices and glass coverslips were washed with deionized water

and isopropyl alcohol, and then treated in a plasma cleaner (Harrick Plasma) for 5 minutes. PDMS

pieces were then bound to activated coverslips and then heated at 95°C on a hotplate for 1 minute

to improve adhesion. After heating, devices were filled with 70% ethanol to sterilize internal

surfaces, rinsed with PBS, and then coated with extracellular matrix proteins. For MDA-MB-231

cells, devices were coated with 50 µg/mL type-I rat tail collagen (Corning) in 0.02 N glacial acetic

acid overnight at 4°C. For MEFs and HT1080 cells, devices were coated with 50 µg/mL fibronectin

(Millipore) in PBS overnight at 4°C. Before seeding with cells, devices were rinsed once with PBS

and once with cell media. Devices were then aspirated of all media, and then loaded with cell-

containing solution (roughly 20,000-30,000 cells per chamber). In devices, cells were cultured in

Fluorobrite DMEM supplemented with 10% FBS (Seradigm, VWR), penn/strep (50 U/mL,

ThermoFisher), GlutaMAX, and 10 mM HEPES (Gibco). Cells were allowed to attach within

devices for 8-12 hours before live cell imaging. Cells were imaged for 12-14 hours at 3-to-5-minute

intervals on a Zeiss LSM700 laser scanning confocal microscope at 37°C.

Collagen Matrix Cell Migration Assay

Collagen matrix cell migration assays were performed as previously described (Cross et al.,

2010). In brief, PDMS wells were formed by punching out 10 mm diameter holes from PDMS

slices. PDMS and glass coverslips were treated in a plasma cleaner for 5 minutes, before bonding

PDMS to treated glass slides on a 95°C hot plate for 3 minutes. Wells were coated with 1% PIE

for 10 minutes, followed by 0.1% Glutaraldehyde for 30 minutes, and then subsequently washed

with PBS once, and cell media once, before adding the collagen solution. Collagen matrices were

prepared by mixing Type I rat tail collagen (Corning) with DMEM and NaOH (to reach a neutral

pH of 7.4) with a solution of cells suspended in complete DMEM to achieve a final density of

80,000 cells/mL. Small volumes of collagen solution (10-15 µL) were pipetted into the middle of

wells, where they were allowed to polymerize at 37°C for 30 minutes. Following polymerization,

577 wells were filled with complete DMEM and were subsequently incubated at 37°C for 48 hours

578 before imaging experiments.

580 ***Laser Alation of Actin***

582 Cells were seeded into migration devices 12-16 hours before ablation experiments. Cells were

583 maintained at 37°C in Fluorobrite DMEM containing 10% FBS, 10 mM HEPES (Gibco), GlutaMax,

584 and penicillin and streptomycin (50 U/mL). Cells were imaged through a water immersion 40×/NA

585 1.1 objective (Carl Zeiss Imaging) using 488-nm and 561-nm laser lines. Cells were imaged at 3

586 second intervals for 63 frames. After 9 seconds, cells were ablated in defined regions using a 780

587 nm laser produced by a Spectra Physics Insight multiphoton excitation source. Ablation was

588 performed at 40-70% attenuation, following ablation tests at the beginning of each experiment to

589 verify that the laser successfully disrupted the actin cytoskeleton without causing cell death. Cells

590 which exited the constriction, displayed rapid blebbing, or appeared to die following laser ablation

591 were excluded from analysis, while cells which were able to recover following disruption of the

592 actin network were included.

594 ***Image Analysis of Laser Ablation Experiments***

595 Tracking of nuclear movement following laser ablation was achieved using ImageJ/FIJI software

596 and a custom MATLAB script. Briefly, the image channel containing the fluorescent mNeonGreen-

597 H2B Histone signal was processed using a 3-pixel median filter to eliminate noise, and then a

598 binary mask of this signal was generated using ImageJ/FIJI's built-in RenyiEntropy masking

599 function. This binary mask was then processed in MATLAB to track the position of the nucleus'

600 centroid at each time point. The furthest position of nuclear movement prior to recovery (within 20

601 seconds of the initial ablation) was considered as the direct result of force disruption as a

602 consequence of laser ablation and was recorded as the peak centroid shift (**Supp. Fig. S6D**).

603 Bleb area measurements were performed in ImageJ/FIJI at the time point when the bleb had

reached its maximum size. Outer bleb perimeter was traced manually, and inner bleb perimeter

was traced at the periphery of the cell at the time point immediately prior to laser ablation.

RhoA FRET Imaging and Analysis

Analysis of RhoA-FRET biosensors was performed as described previously (Cheung et al., 2022).

Cells were imaged at regular intervals on a dual channel image acquisition set-up to minimize

temporal and spatial misalignment problems which impair FRET result interpretation. Cells were

imaged at 5-minute intervals for 12 to 16 hours. Cells were excited with a ET436/20× (CFP

Excitation) source for an exposure time of 3 seconds with CFP excitation while CFP and YFP

("FRET") emission channels were captured simultaneously, by using a W-View Gemini beam

splitter (A12801-01, Hamamatsu Photonics) and a T505lpxr dichroic mirror, through ET480/40m

and ET535/30m optical filters, respectively. The light source for fluorescence imaging was a

xenon arc lamp (Lambda LB-LS/30, Sutter Instruments). An absorptive neutral density filter with

OD = 0.3 (NE03B-A, ThorLabs) was used to attenuate light to minimize phototoxicity. All filters

and dichroic mirrors were purchased from Chroma Technology. Prior to each experiment, the x-

y positions of CFP and FRET channels were adjusted using the W-VIEW Adjustment software

(Hamamatsu Photonics) to achieve a reasonable alignment for easier image registration and

processing. The epifluorescence microscope was surrounded by an incubator with a temperature

of 37°C, 5% CO_2, and humidity of ~70%.

Field alignment, flatfield correction, and background subtraction were performed as described

previously (Cheung et al., 2022). Images of cells were then manually masked by tracing the

outline of cells using the CFP channel in FIJI/ImageJ. Following these corrections to both the CFP

and FRET channels, FRET ratios were calculated by dividing the FRET channel by the CFP

channel. The sensitivity of the RhoA-FRET biosensor expressed in this MDA-MB-231 cell line to

RhoA activation and inactivation was performed under identical experimental conditions on this

imaging set-up as described previously (Cheung et al., 2022). Local FRET ratios were then

calculated by manually tracing regions as defined in Supp. Fig. S5A.

Analysis of Migration Mode and Nuclear Transit Times

Measurements of nuclear transit times were performed as described previously (Davidson et al.,

2015). Briefly, cells were imaged at 5-minute intervals on a Zeiss LSM710 laser scanning confocal

microscope using 488-nm and 561-nm laser lines as they migrated through migration devices

over a period of 12-16 hours. A fluorescent marker of the nucleus (either mNeonGreen-H2B

Histone, or GFP-Nesprin2) was used to track the position of the nucleus relative to microfluidic

constrictions. An imaginary line 5 microns was marked on either side of the middle of the

constriction, to define when the nucleus "enters" and "exits" the constriction. The times at which

the nucleus enters and passes through the constriction were noted, and this interval was recorded

as the nuclear transit time. Cells which did not complete nuclear transit following entry to the

constriction were excluded from analysis.

Immunofluorescence Imaging

Cells were fixed in PDMS microfluidic devices using a solution of 4% Paraformaldehyde on ice

for 10 minutes, washed twice with PBS for 5 minutes, permeabilized with 0.2% Triton in PBS at

room temperature, blocked with a solution of Bovine Serum Albumin (3% v/v) with 0.05% Tween

and 0.2% Triton in PBS for 1 hour, and then treated with primary antibodies (anti-pMLC, cell

signaling 1:100) in blocking solution overnight at 4°C. Cells were then washed 3 times with PBS

for 10 minutes each, and then treated with Secondary Antibodies (Alexa Fluor 488 anti-Rabbit),

Phalloidin 647 (1:400 dilution), and Hoechst (1:5000 dilution) for 2 hours at room temperature.

Cells were washed 3 times with PBS for 10 minutes each. Devices were filled with blocking

solution and sealed with glass coverslips prior to imaging.

Statistical Analysis

All experimental data are based on at least three independent experiments, unless otherwise

specified. Statistics tests were performed and graphs were created using GraphPad Prism

(GraphPad Software, San Diego, USA). Nuclear transit times were compared using a one-way

ANOVA. Frequency of nuclear transit mechanism selection was performed using a Chi Squared

test of independence. Changes in local FRET ratio during nuclear transit were evaluated using a

paired non-parametric ANOVA test (Wilcoxon). Nuclear centroid shifts following laser ablation

were compared using an unpaired non-parametric ANOVA test (Kruskal-Wallis). Bleb formation

in cells ablated at a single site were compared using an unpaired non-parametric ANOVA test

(Kruskal-Wallis) while bleb formation in cells ablated at both cortexes simultaneously were

compared using a paired non-parametric ANOVA test (Wilcoxon).

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Competing Interests

The authors declare no competing interests. Jan Lammerding has received consulting fees from

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References

Bone, C.R., Chang, Y.T., Cain, N.E., Murphy, S.P., Starr, D.A., 2016. Development 143, 4193–4202.

Caille, N., Thoumine, O., Tardy, Y., Meister, J.J., 2002. J Biomech 35, 177–187.

Charras, G.T., Yarrow, J.C., Horton, M.A., Mahadevan, L., Mitchison, T.J., 2005. Nature 435, 365–369.

Cheung, B.C.H., Hodgson, L., Segall, J.E., Wu, M., 2022. Experimental Cell Research 410, 112939.

Cross, V.L., Zheng, Y., Won Choi, N., Verbridge, S.S., Sutermaster, B.A., Bonassar, L.J., Fischbach, C., Stroock, A.D., 2010. Biomaterials 31, 8596–8607.

Davidson, P.M., Battistella, A., Déjardin, T., Betz, T., Plastino, J., Borghi, N., Cadot, B., Sykes, C., 2020. EMBO Rep 21, e49910.

Davidson, P.M., Denais, C., Bakshi, M.C., Lammerding, J., 2014. Cellular and Molecular Bioengineering 7, 293–306.

Davidson, P.M., Sliz, J., Isermann, P., Denais, C.M., Lammerding, J., 2015. Integr Biol 7, 1534–1546.

Denais, C.M., Gilbert, R.M., Isermann, P., McGregor, A.L., te Lindert, M., Weigelin, B., Davidson, P.M., Friedl, P., Wolf, K., Lammerding, J., 2016. Science (1979) 352, 353–358.

Doyle, A.D., Petrie, R.J., Kutys, M.L., Yamada, K.M., 2013. Curr Op Cell Bio 25, 642–649.

Friedl, P., Wolf, K., 2010. Journal of Cell Biology 188. 11-19

Gadea, G., de Toledo, M., Anguille, C., Roux, P., 2007. Journal of Cell Biology 178, 23–30.

Geiger, F., Rüdiger, D., Zahler, S., Engelke, H., 2019. PLoS ONE 14.

Geum, D., Kim, B., Chang, A., Hall, M., Wu. M., 2016. European Physical Journal Plus.

Harada, T., Swift, J., Irianto, J., Shin, J.-W., Spinler, K.R., Athirasala, A., Diegmiller, R., Dingal, P.C.D.P., Ivanovska, I.L., Discher, D.E., 2014. Journal of Cell Biology 204, 669–682.

Hetmanski, J.H.R., de Belly, H., Busnelli, I., Waring, T., Nair, R. v, Sokleva, V., Dobre, O., Cameron, A., Gauthier, N., Lamaze, C., Swift, J., del Campo, A., Starborg, T., Zech, T., Goetz, J.G., Paluch, E.K., Schwartz, J.-M., Caswell, P.T., 2019. Developmental Cell 51, 460-475.e10.

Jayo, A., Malboubi, M., Antoku, S., Chang, W., Ortiz-Zapater, E., Groen, C., Pfisterer, K., Tootle, T., Charras, G., Gundersen, G.G., Parsons, M., 2016. Dev Cell 38, 371–383.

Keys, J., Windsor, A., Lammerding, J., 2018. Assembly and Use of a Microfluidic Device to Study Cell Migration in Confined Environments, in: Gundersen, G.G., Worman, H.J. (Eds.), The LINC Complex: Methods and Protocols. Springer New York, New York, NY, pp. 101–118.

Khatau, S.B., Bloom, R.J., Bajpai, S., Razafsky, D., Zang, S., Giri, A., Wu, P.H., Marchand, J.,
Celedon, A., Hale, C.M., Sun, S.X., Hodzic, D., Wirtz, D., 2012. Sci Rep 2.

Lammerding, J., 2011. Compr Physiol 1, 783–807.

Lämmermann, T., Bader, B.L., Monkley, S.J., Worbs, T., Wedlich-Söldner, R., Hirsch, K., Keller,
M., Förster, R., Critchley, D.R., Fässler, R., Sixt, M., 2008. Nature 453, 51–55.

Lee, H., Alisafaei, F., Adebawale, K., Chang, J., Shenoy, V.B., Chaudhuri, O., 2021. Science
Advances 7, eabd4058.

Liu, Y.-J., Le Berre, M., Lautenschlaeger, F., Maiuri, P., Callan-Jones, A., Heuzé, M., Takaki, T.,
Voituriez, R., Piel, M., 2015. Cell 160, 659–672.

Marks, P.C., Petrie, R.J., 2022. Phys Biol 19.

McGregor, A.L., Hsia, C., Lammerding, J., 2016. Curr Op Cell Bio 40, 32–40.

Mistriotis, P., Wisniewski, E.O., Bera, K., Keys, J., Li, Y., Tuntithavornwat, S., Law, R.A., Perez-
Gonzalez, N.A., Erdogmus, E., Zhang, Y., Zhao, R., Sun, S.X., Kalab, P., Lammerding, J.,
Konstantopoulos, K., 2019. J Cell Biol 218, 4093–4111.

Pertz, O., Hodgson, L., Klemke, R.L., Hahn, K.M., 2006. Nature 440, 1069–1072.

Petrie, R.J., Harlin, H.M., Korsak, L.I.T., Yamada, K.M., 2016. Journal of Cell Biology 216, 93–
100.

Petrie, R.J., Koo, H., Yamada, K.M., 2014. Science (1979) 342, 1062–1065.

Poincloux, R., Collin, O., Lizárraga, F., Romao, M., Debray, M., Piel, M., Chavrier, P., 2011.
Proceedings of the National Academy of Sciences 108, 1943–1948.

Rowat, A.C., Jaalouk, D.E., Zwerger, M., Ung, W.L., Eydelnant, I.A., Olins, D.E., Olins, A.L.,
Herrmann, H., Weitz, D.A., Lammerding, J., 2013. Journal of Biological Chemistry 288,
8610–8618.

Sahai, E., Marshall, C.J., 2003. Nat Cell Biol 5, 711–719.

Schaar, B.T., McConnell, S.K., 2005. PNAS 102.

Thiam, H.R., Vargas, P., Carpi, N., Crespo, C.L., Raab, M., Terriac, E., King, M.C., Jacobelli, J.,
Alberts, A.S., Stradal, T., Lennon-Dumenil, A.M., Piel, M., 2016. Nature Communications 7.

Thomas, D.G., Yenepalli, A., Denais, C.M., Rape, A., Beach, J.R., Wang, Y.-L., Schiemann,
W.P., Baskaran, H., Lammerding, J., Egelhoff, T.T., 2015. J Cell Biol 210, 583–594.

Tinevez, J.-Y., Schulze, U., Salbreux, G., Roensch, J., Joanny, J.-F., Paluch, E., 2009.
Proceedings of the National Academy of Sciences 106, 18581–18586.

Tollis, S., Rizzotto, A., Pham, N.T., Koivukoski, S., Sivakumar, A., Shave, S., Wildenhain, J.,
Zuleger, N., Keys, J.T., Culley, J., Zheng, Y., Lammerding, J., Carragher, N.O., Brunton,
V.G., Latonen, L., Auer, M., Tyers, M., Schirmer, E.C., 2022. ACS Chemical Biology 17,
680–700.

Tsai, J.W., Lian, W.N., Kemal, S., Kriegstein, A.R., Vallee, R.B., 2010. Nature Neuroscience 13,
1463–1472.

Weigelin, B., Bakker, G.-J., Friedl, P., 2012. IntraVital 1, 32–43.

Wolf, Katarina, te Lindert, M., Krause, M., Alexander, S., te Riet, J., Willis, A.L., Hoffman, R.M.,
Figdor, C.G., Weiss, S.J., Friedl, P., 2013. Journal of Cell Biology 201, 1069–1084.

Wolf, K, te Lindert, M., Krause, M., Alexander, S., te Riet, J., Willis, L.A., Hoffman, R.M., Figdor,
C.G., Weiss, S.J., Friedl, P., 2013. J Cell Biol 201, 1069–1084.

Wolf, K., Mazo, I., Leung, H., Engelke, K., von Andrian, U.H., Deryugina, E.I., Strongin, A.Y.,
Bröcker, E.B., Friedl, P., 2003. Journal of Cell Biology 160, 267–277.

Yadav, S.K., Feigelson, S.W., Roncato, F., Antman-Passig, M., Shefi, O., Lammerding, J., Alon,
R., 2018. Journal of Leukocyte Biology 104, 239–251.

Yamada, K.M., Sixt, M., 2019. Nature Reviews Molecular Cell Biology 20, 738–752.