

Nanobody engineering for SARS-CoV-2 neutralization and detection

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1 **Abstract**

2 In response to the ongoing SARS-CoV-2 pandemic, the quest for coronavirus inhibitors has
3 inspired research on a variety of small proteins beyond conventional antibodies, including
4 robust single-domain antibody fragments, ‘nanobodies’. Here, we explore the potential of
5 nanobody engineering in the development of antivirals and diagnostic tools. Through fusion of
6 nanobody domains that target distinct binding sites, we engineered multimodular nanobody
7 constructs that neutralize wild-type SARS-CoV-2 and the Alpha and Delta variants with high
8 potency, with IC₅₀ values up to 50 pM. However, we observed a limitation in the efficacy of
9 multimodular nanobodies against the Beta (B.1.351) and Omicron variants (B.1.1.529),
10 underlining the importance of accounting for antigenic drift in the design of biologics. To
11 further explore the applications of nanobody engineering in outbreak management, we present
12 a novel diagnostic assay, based on fusions of nanobodies with fragments of NanoLuc luciferase
13 that can detect sub-nanomolar quantities of the SARS-CoV-2 spike protein in a single step.
14 Our work showcases the potential of nanobody engineering to combat emerging infectious
15 disease.

16

17 **Introduction**

18 Antibody-based products comprise some of the most successful diagnostic and therapeutic
19 tools developed for managing the COVID-19 pandemic, ranging from at-home rapid antigen
20 tests for SARS-CoV-2 infection (1, 2) to neutralizing monoclonal antibodies (mAbs) used to
21 treat COVID-19 in individuals at risk of severe disease (2, 3). Neutralizing antibodies against
22 SARS-CoV-2 primarily target the Spike (S) protein (4, 5), a glycoprotein that mediates host-
23 cell recognition and viral entry (6). SARS-CoV-2 spikes are homotrimers, with each S chain
24 consisting of receptor-binding (S1) and fusogenic (S2) subunits (7). The S1 subunit contains

25 the receptor-binding domain (RBD) which mediates binding to the primary cellular receptor of
26 SARS-CoV-2, angiotensin-converting enzyme 2 (ACE2) (6, 8, 9). Following receptor binding,
27 the S2 subunit, a class I fusion protein, is activated by proteolytic cleavage and mediates the
28 fusion of the viral and cell membranes, delivering viral RNA to the cytoplasm (8, 10).

29 Due to its key role in initiating infection, the SARS-CoV-2 spike is the primary target of both
30 vaccines (11) and monoclonal antibody therapy (2). The continued efficacy of these powerful
31 approaches is challenged by the emergence of SARS-CoV-2 variants of concern (VOCs) that
32 display multiple amino acid substitutions in the S-protein (12-14). Following the spread of
33 variants Alpha (B.1.1.7), Beta (B.1.351) and Delta (B.1.617.2) (15-20), Omicron (B.1.1.529)
34 has become established as the dominant circulating variant in 2022, with new Omicron sub-
35 variants still emerging (21). VOC amino acid changes, including E484K found in Beta and
36 Omicron, can significantly reduce neutralization by antibodies raised against the ‘wild-type’
37 SARS-CoV-2 (titled B.1 or Wuhan-Hu-1) (12, 15, 16, 19, 22). Current efforts to mitigate the
38 effects of immune escape on antibody-based COVID-19 countermeasures include the use of
39 antibody cocktails (23, 24) and the development of new antibody-based products, including
40 camelid single-domain antibody fragments (‘nanobodies’) (25).

41 In contrast to traditional mAbs, nanobodies are small (~15 kDa) and offer many advantages
42 including nebulized delivery and scalable, cost-effective production in bacterial expression
43 systems (26, 27). During the COVID-19 pandemic, antiviral nanobodies have garnered
44 significant interest, resulting in the discovery and structural characterization of several SARS-
45 CoV-2-neutralizing nanobodies (27-37). Furthermore, as nanobodies comprise self-contained
46 modules, they can be engineered into fusion proteins with enhanced properties. Pioneering
47 studies have started to chart the potential of engineered nanobodies as virus inhibitors (38, 39),
48 but their diagnostic applications are largely unexplored. While RT-qPCR remains the gold
49 standard for clinical diagnosis, rapid diagnostic tests designed to detect viral antigens with

50 conventional antibodies (40) are extensively applied in nonhospital settings. To our knowledge,
51 nanobodies have not, so far, been used for viral antigen detection in commercialized assays.
52 Here, we explore an engineering strategy that leverages nanobody fusions for enhanced
53 neutralization and in the development of a novel rapid-antigen assay. Tri-modular fusions of
54 selected nanobodies showed up to a hundredfold enhancement of the *in vitro* neutralization
55 efficiency against wild-type SARS-CoV-2 as compared to the reported efficiencies of the
56 single constituent nanobodies (28-30, 41). We suggest that molecular dynamics (MD)
57 simulations can be used to analyze the neutralization potential of nanobodies against VOCs, of
58 which Beta and Omicron escaped neutralization, and offer a possible mechanistic explanation
59 for the neutralization escape. Nanobody fusions were further engineered to produce proof-of-
60 concept for a novel diagnostic assay, which applies nanobodies fused to fragments of a split
61 signal molecule, NanoLuc luciferase (42-44), and allows the detection of picomolar
62 concentrations of SARS-CoV-2 spike protein in a single step. Overall, our study shows the
63 potential for engineered nanobodies as antiviral and diagnostic agents, which we envision can
64 offer affordable and scalable countermeasures during future outbreaks of emerging viral
65 diseases.

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67 **Results**

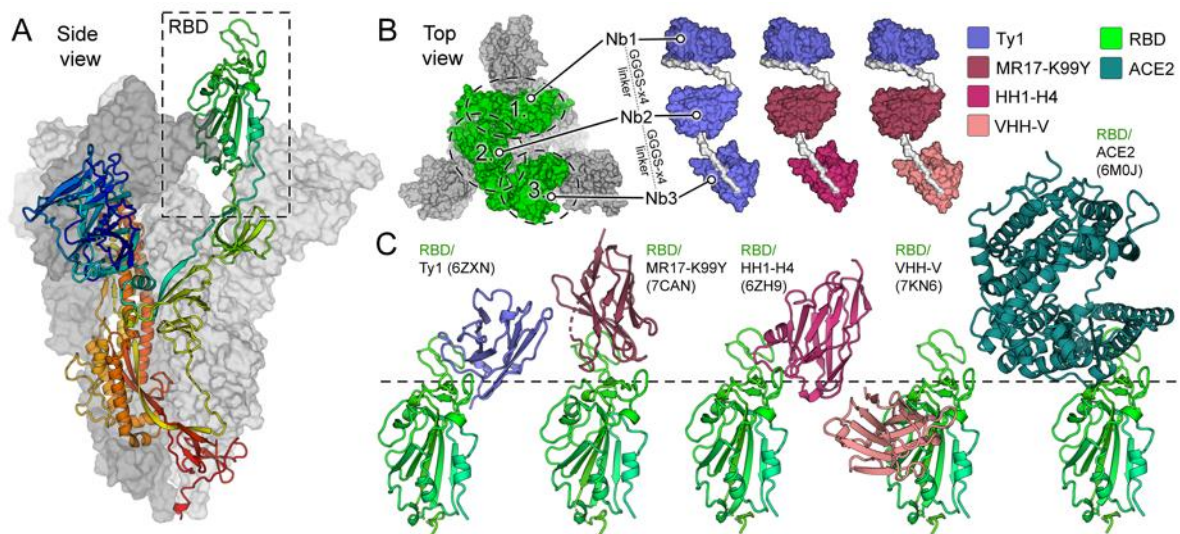
68 **Structure-guided design of multimodular nanobodies.** Structural studies have elucidated
69 key sites of vulnerability on SARS-CoV-2 (4, 45), including an ACE2-receptor binding
70 interface that can be targeted to sterically hinder receptor engagement (46-48). Inspired by the
71 trimeric structure of the coronaviral spike (Figure 1), we sought to develop an approach for
72 targeting all three copies of RBD simultaneously to enhance SARS-CoV-2 inhibition.
73 Cryogenic electron microscopy (cryo-EM) studies have identified two distinct SARS-CoV-2

74 RBD conformations, titled ‘up’ and ‘down’ (49, 50), where putative epitopes on neighboring
75 RBDs are in proximity, within 40 to 74 Å from each other (SI Figure S1). To develop a tripartite
76 binder that could be sterically accommodated within these tight constraints, we selected
77 nanobodies, the smallest antibody-based protein inhibitors, as the base unit for
78 multimodularization.

79 We designed three trimodular nanobodies (Figure 1B) using the sequences of four previously
80 published monomeric nanobodies, Ty1 (47), H11-H4 (29), MR17-K99Y (30) and VHH V (41).
81 These modules were selected based on two criteria: (i) distinct epitope and angle of binding to
82 RBD (Figure 1C and SI Table S1), (ii) spatial proximity of the epitopes in the context of the
83 SARS-CoV-2 spike, facilitating the simultaneous binding of all modules (Figure 1). While each
84 individual module has been reported to neutralize wild-type SARS-CoV-2 with IC₅₀ (half-
85 maximal inhibitory concentration) values ranging from 40 to 142 nM (SI Table S1), our
86 multimodularization approach was designed to improve neutralization potency through
87 increased avidity to the SARS-CoV-2 spike, and to test whether multimodular constructs can
88 neutralize variants of concern.

89 Multimodular nanobodies were constructed by fusing multiple nanobodies together with
90 flexible linkers of twenty amino acids (GGGGs_{x4}) with the aim to improve the binding avidity
91 (26, 39, 51-53). Furthermore, as modules targeting distinct epitopes can be included in the same
92 construct, multimodularization has been proposed to reduce neutralization escape resulting
93 from amino acid changes in viral proteins (41). Here, construct compositions were selected to
94 test i) the effect of triplicating a single module (tri-Ty1, comprised of three Ty1 modules (47))
95 on SARS-CoV-2 neutralization, and ii) whether the inclusion of variable modules can help
96 mitigate neutralization escape by virus variants (41). To this end, multimodular constructs tri-
97 Ty1, tri-TMH, and tri-TMV (Figure 1B) were generated, with tri-TMH and tri-TMV comprised
98 of Ty1 (47) and MR17-K99Y (30) modules, followed by either a H11-H4 (29) or VHH V (41)

99 module, respectively. Tri-Ty1, tri-TMH, and tri-TMV readily expressed in *E.coli*, and were
100 purified and enrolled in target binding and virus neutralization assays.



101

102 **Figure 1. Structure-based design of multimodular nanobodies targeting SARS-CoV-2 S.**
103 **A)** Side view of the SARS-CoV-2 S-trimer (47). One trimer subunit, with a receptor-binding
104 domain (RBD), in the 'up' conformation, is shown as a cartoon and colored as a rainbow
105 ramped from blue (N-terminus) to red (C-terminus). The two other subunits are shown as
106 surface representation in shades of grey. **B)** Three distinct multimodular nanobodies were
107 designed: (i) tri-Ty1 with three repeats of Ty1 (47) module; (ii) tri-TMH with Ty1, MR-17-
108 K99Y (30) and HH1-H4 (29) modules; and (iii) Tri-TMV with Ty1, MK and VHH-V (41)
109 modules. The nanobody modules are connected by flexible GGGGSx4 linkers. **C)** Each of the
110 nanobody domains (Ty1, MR17-K99Y, HH1-H4, and VHH-V) bind the RBD at a unique
111 angle. Comparison to the structure of RBD bound to the primary host-cell entry receptor of
112 SARS-CoV-2, ACE2 (6, 54) demonstrates that three of the modules bind epitopes proximal to
113 the ACE2-binding site, while VHH-V targets an alternative neutralization epitope.

114

115 **Multimodular nanobodies bind variant forms of the RBD.** Amino acid changes observed
116 in SARS-CoV-2 variants of concern have been linked to escape from antibody-mediated virus
117 neutralization (15, 16, 55, 56) due to reduced affinity to epitopes where key amino acids have
118 been altered. To determine how prominent RBD amino acid changes K417N, E484K, and
119 N501Y impact the binding of trimodular nanobodies, we tested their binding to RBD and spike
120 mutants in an antigen microarray. Nanobodies tri-Ty1, tri-TMH, and tri-TMV were tested
121 against (i) wild-type RBD, (ii-iv) three RBD variants that displayed either K417N, E484K, or

122 N501Y amino acid change, (v) wild-type S1 subunit, and (vi) a S1 subunit displaying the amino
123 acid changes K417N, E484K, N501Y, and D614G. Multimodular tri-TMH and tri-TMV
124 constructs contain nanobody modules that target three epitopes comprising a broad range of
125 residues, and as such, these constructs were expected to be less sensitive to amino acid changes
126 than the single-module tri-Ty1. The results support this hypothesis, showing that the binding
127 of tri-Ty1 to the RBD was strongly diminished by the E484K change, while this effect was
128 mitigated in tri-TMH and tri-TMV (Figure 2). Amino acid changes K417N or N501Y did not
129 significantly alter the binding affinity on any of the nanobody constructs.

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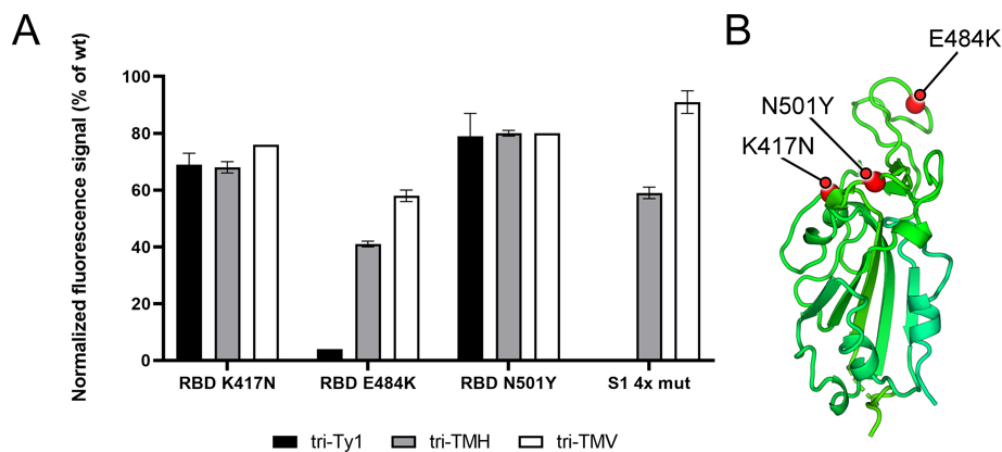
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138 **Figure 2. Relative binding strength of trimeric nanobodies to different RBD and Spike S1**
139 **domain variants on the antigen microarray. A)** Three multimodular nanobody constructs
140 were tested in a binding array and were shown to bind different RBD or S1 domain variants.
141 Binding of tri-Ty1 was obstructed by the amino acid change E484K, which is found in the Beta
142 VOC and linked to neutralization escape (12, 16, 55) The multimodular nanobodies comprised
143 of modules that target distinct epitopes, tri-TMH and tri-TMV, retained a level of binding to
144 the E484K RBD variant. The fluorescence signals of Dylight 633-labelled trimeric nanobodies
145 tri-Ty1, tri-TMH and tri-TMV bound to the different RBD and S1 mutants in the array were
146 normalized relative to the corresponding wt protein signals in the same array. Error bars
147 represent the standard deviation of two replicate wells. **B)** Location of the amino acid changes
148 within the SARS-CoV-2 RBD in the Alpha and Beta variants. Amino acid change N501Y is
149 found in the Alpha and Beta variants (15, 16), and the Beta variant displays the additional
150 changes K417N and E484K (16).

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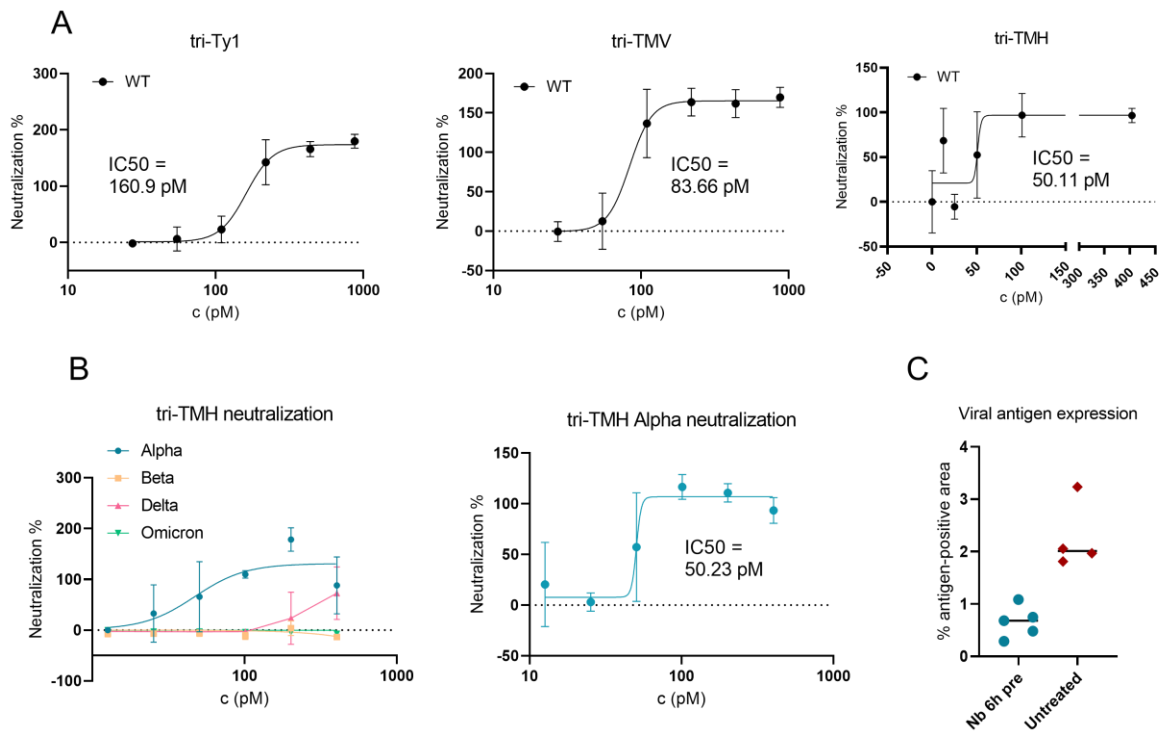
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153 **Multimodular nanobodies potently neutralize SARS-CoV-2 wild-type and Alpha.**

154 Multimodular nanobodies targeting SARS-CoV-2 S trimer were designed to increase
155 neutralization efficacy over single module nanobodies via enhanced avidity. In addition, the
156 ability of multimodular nanobodies to target distinct epitopes was expected to reduce
157 neutralization escape by emerging variants. To test these hypotheses, we determined the
158 neutralization potency of multimodular nanobodies against SARS-CoV-2 variants *in vitro*,
159 using a plaque-reduction neutralization assay in VeroE6-TMPRSS2 cells (Figure 3). All
160 multimodular nanobodies neutralized wild-type virus (50 pfu) at ultra-high potency, with IC50
161 values ranging from 160.9 pM for tri-Ty1, to 83.66 pM for tri-TMV and 50.11 pM for tri-TMH.
162 This result shows that the multimodular structure improves neutralization efficacy from the
163 single constituent nanobodies up to hundred-fold, which is in line with recent works presenting
164 similar, significant increase in neutralization potency over single module nanobodies (38, 41,
165 57, 58). Neutralization was also tested with virus administered at 1 MOI, where the relative
166 efficacies of the nanobodies followed the same trends as in the 50 pfu assay, although at
167 somewhat lower IC50-values ranging from 400 pM to 2 nM (SI Figure S5).

168 To investigate the capability of multimodular nanobodies to neutralize SARS-CoV-2 variants
169 of concern, we tested tri-TMH, the most potent neutralizer of wild-type SARS-CoV-2 among
170 our designs, against the wide-spread variants of concern Alpha, Beta, Delta, and Omicron. Tri-
171 TMH neutralizes SARS-CoV-2 Alpha variant with equivalent potency to wild-type (IC50 =
172 50.23 pM), and Delta with declined potency (estimated IC50 ~600 pM). The Beta and Omicron
173 variants, however, escaped neutralization by multimodular nanobodies (Figure 3B). We
174 hypothesize that the reduction of neutralization potency against Beta and Omicron arises from
175 the well-known neutralization escape mutation E484K, which is present in the Beta and
176 Omicron variants, but not in wild-type or the other variants studied. This contrasts with the
177 antigen microarray data (Figure 2), where nanobodies with three distinct modules were found

178 to retain most of their binding to RBD with this mutation. While neutralization is observed for
179 the Delta variant, the potency of tri-TMH against delta is reduced, presumably due to the other
180 changes in Delta, such as L452R, which has been linked to neutralization escape from
181 antibodies (19, 59).



182 **Figure 3. Multimodular nanobodies neutralize SARS-CoV-2 wild-type, Alpha and Delta**
183 **variants at high potency and limit the course of the disease in a hamster model. A)** Wild-
184 **type SARS-CoV-2 is neutralized by nanobodies tri-Ty1, tri-TMV, and tri-TMH. B)** Tri-TMH
185 **neutralizes the Alpha and Delta variants. C)** A morphometric analysis of the presence of SARS-
186 **CoV-2 antigens in lung tissue sections shows a decrease in viral antigen expression in hamsters**
187 **pre-treated with multimodular nanobody (Nb 6h pre), compared to untreated individuals (n =**
188 **5 in nanobody treated group, n = 4 in untreated).**

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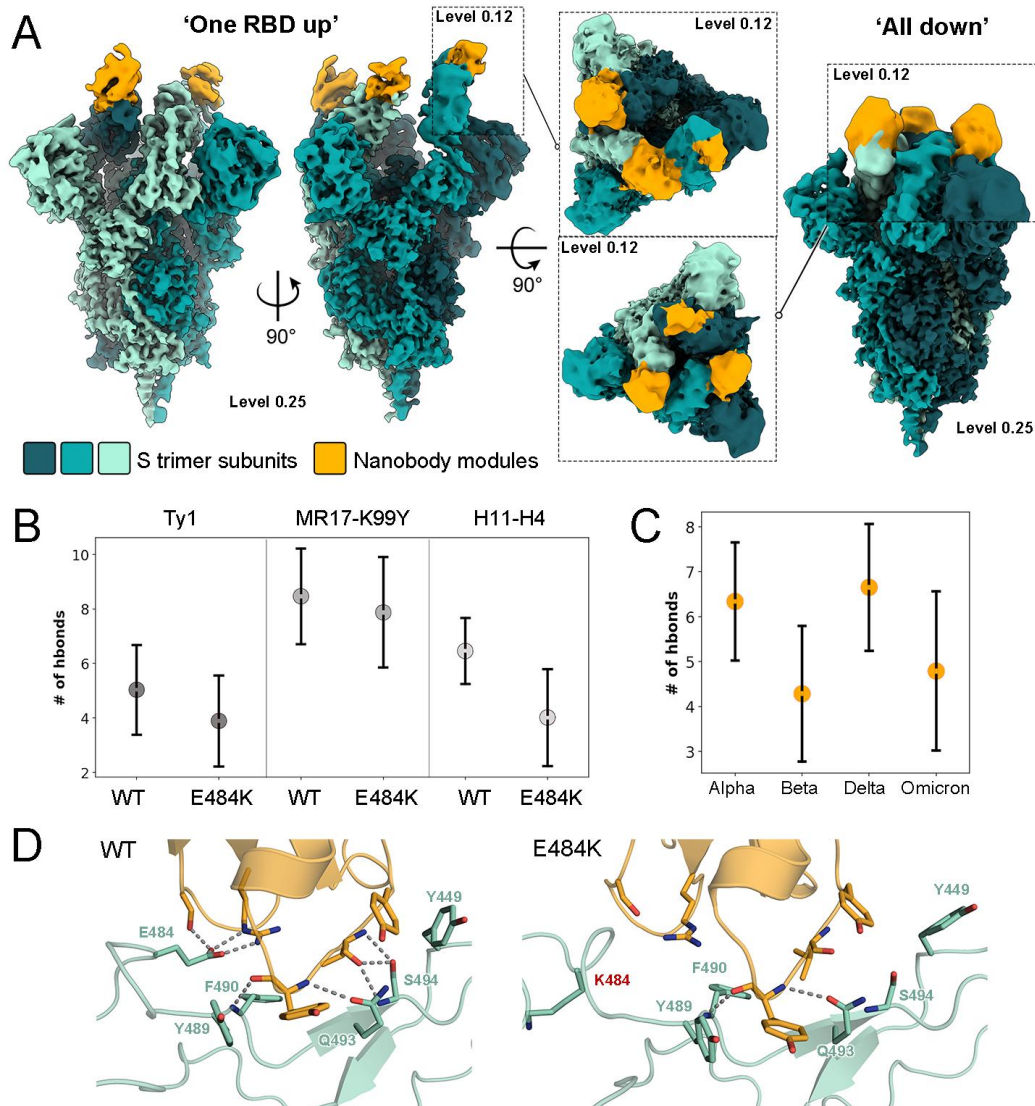
194 **Cryo-EM analysis reveals the conformational landscape of SARS-CoV-2 spike bound to**
195 **a multimodular nanobody.** While many individual nanobody modules and their binding
196 epitopes on the S protein have been structurally characterized, these reconstructions may be
197 incommensurate to linker-connected multimodular nanobody constructs, as they do not
198 account for the potential steric constraints imposed by linker-bound modules (29-37, 47). As
199 such, the effects of multimodularity in S-targeting nanobodies on nanobody neutralization
200 mechanisms remain largely unexplored. We applied cryo-EM to determine the binding mode
201 of multimodular nanobody tri-TMH to SARS-CoV-2 S protein.

202 The receptor-binding domains of SARS-CoV-2 spike transition between states designated “up”
203 and “down”, of which the “up” conformation is accessible to ACE2 receptor binding (4, 7).
204 This natural variation leads to the presence of distinct subpopulations in cryo-EM data, where
205 the conformational landscape is primarily comprised of fully closed (“all down”) and partially
206 open (“2 down, 1 up”) states (4, 7, 60). While differential distributions of the two states have
207 been reported, native spikes on viral surface show 31% and 55% of fully closed and partially
208 open conformations, respectively (60). Furthermore, certain neutralizing antibodies have been
209 shown to disrupt the conformation of the spike due to steric incompatibility with the prefusion
210 state (61, 62).

211 We set out to determine how nanobody tri-TMH impacts the conformation of the spike. Our
212 cryo-EM data showed that the spike retained a prefusion conformation with subpopulations
213 presenting the closed and partially open states. Both states are fully bound with tri-TMH
214 (Figure 4A), although due to the variable placement of the modules, local resolution does not
215 allow the unambiguous identification of individual nanobody moieties. Our results indicate that
216 the inclusion of multiple simultaneously binding modules, linked by the commonly used
217 (GGGGS)₄ linker, does not result in sufficient steric strain to disrupt the prefusion
218 conformation, and the linker seems to allow the native distribution of RBD conformational

219 states. We postulate that the increased potency of multimodular inhibitors is primarily derived
220 from enhanced avidity, as opposed to altered mechanistic properties.

221 **Molecular dynamics simulations indicate re-arrangement of nanobody-RBD interface as**
222 **a result of amino acid changes present in VOC.** Following the cryo-EM analysis that
223 validated the conformation of the spike and the RBDs, we sought to elucidate the molecular
224 basis for neutralization evasion as observed for VOC beta (Figure 3) via molecular dynamics
225 (MD) simulations. Interestingly, many nanobodies, as well as antibodies derived from B cells
226 of COVID-19 convalescent and vaccinated individuals, show a salt bridge between an antibody
227 scaffold arginine (R52 in nanobodies) and residue E484 of the RBD (15, 16). As this residue
228 is the site of amino acid change E484K that is linked to neutralization evasion by VOCs (16,
229 22, 63), we sought to determine how E484K impacts the interface of RBD and nanobody
230 modules included in tri-TMH. MD simulations of both WT RBD and E484K RBD were
231 performed with the individual nanobody module monomers.



232

233 **Figure 4. Insights into multimodular nanobody binding from cryo-EM analysis and**
 234 **molecular dynamics simulations.** A) Cryo-EM reconstructions of the S-trimer with
 235 multimodular nanobody tri-TMH bound. The reconstructions show the typical spike protein
 236 conformations (one RBD up and all RBDs down). B) Number of hydrogen bonds between
 237 RBD (wild-type or with E484K amino acid change) and each nanobody module of tri-TMH
 238 observed from MD simulation data. The dot shows the mean value based on all simulation
 239 replicas, and the line represents the standard deviation. C) The number of hydrogen bonds
 240 between nanobody module H11-H4 and the RBD of SARS-CoV-2 VOCs, as predicted by MD
 241 simulations. D) The interface between nanobody module H11-H4 (orange) and wild-type RBD
 242 (green). E) The interface between nanobody module H11-H4 (orange) and RBD (green) with
 243 amino acid change E484K (highlighted in red).

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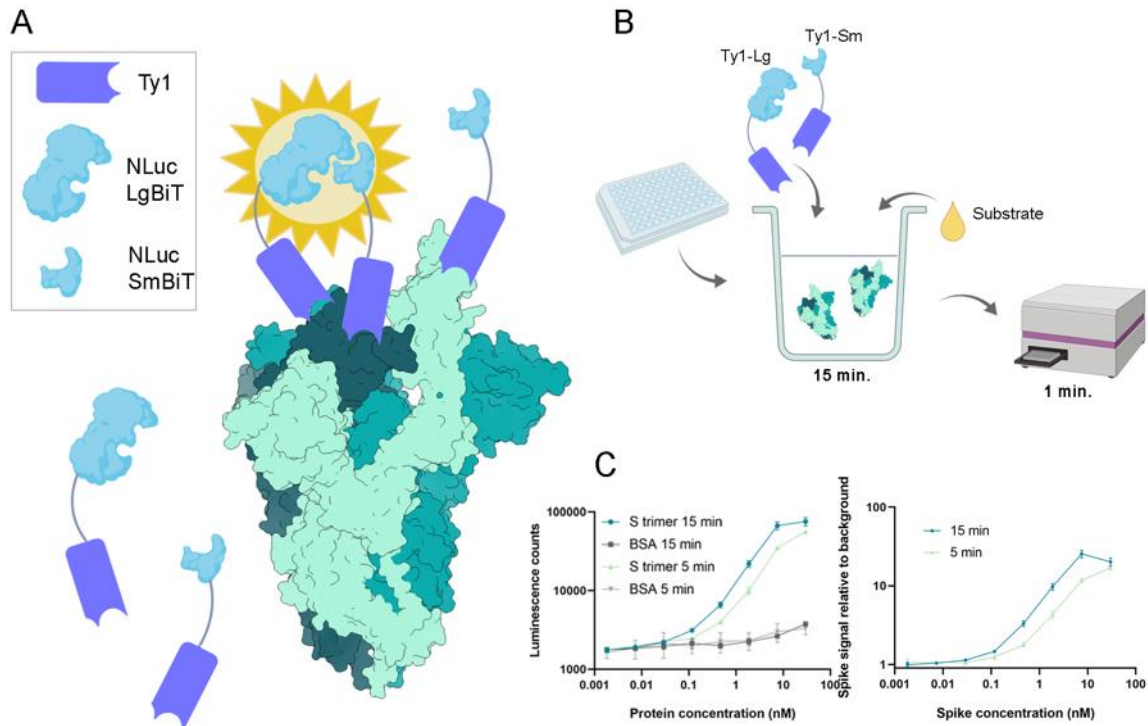
246 For the MR17-K99Y and H11-H4 modules, the R52-E484 salt bridge was identified to be
247 extremely stable throughout the WT simulations and in multiple independent simulation
248 replicas (ca. 95 % of total simulation time). However, when amino acid change E484K was
249 simulated, the interaction to R52 was rapidly broken (within 1 ns). The dissociation of the salt
250 bridge as a consequence of charge change from anionic glutamate to positively charged lysine
251 contributed to higher instability of the E484K RBD, with the surrounding loop becoming more
252 mobile (Figure S2 and S3, Figure 4D-E). In addition, the number of hydrogen bonds between
253 RBD and the nanobody modules decreased in the E484K systems (Figure 4B). The majority of
254 these disrupted hydrogen bonds were identified to be in the conserved RBD binding epitope
255 (Figure 4D-E). Additional model systems were constructed with the full set of VOC mutations
256 in the RBD. Here, the Alpha and Delta VOC, where E484 is preserved, behaved similarly to
257 the WT systems. However, both Beta and Omicron VOC, where E484 is substituted by lysine
258 and alanine respectively, showed higher instability (SI Figure S2) and a decrease in hydrogen
259 bonding interactions throughout the simulation (Figure 4C). These data indicate that E484 is
260 central for strong nanobody binding.

261 **Nanobodies fused to split nanoluciferase fragments detect SARS-CoV-2 Spike at**
262 **picomolar concentrations.** Antibody-based diagnostics are widely used for detecting SARS-
263 CoV-2, as they yield results rapidly and are easy to use in point-of-care and outpatient settings
264 (40). Here, we applied nanobody engineering in the development of a novel SARS-CoV-2
265 detection assay. The modular nature of nanobodies makes them amenable to fusion with signal
266 molecules, and their small size allows the targeting of proximal epitopes, such as those
267 presented by the three subunits of the SARS-CoV-2 spike trimer. These properties align well
268 with the principle of protein-fragment complementation assays, where the activity of a split
269 signal molecule, such as a luciferase, a fluorescent protein, or a betalactamase, is restored once
270 the split fragments are brought into close proximity by the interaction of proteins fused to the

271 fragments (64). Nanobodies shown in Figure 1 target epitopes in the RBD, and we
272 hypothesized that, when fused to split signal molecule fragments, their binding to the three
273 spike subunits will reconstitute the signal molecule, potentially allowing sensitive detection in
274 a single step.

275 Here, we selected the split version of NanoLuc, an engineered 19-kDa luciferase with enhanced
276 stability and brightness compared to the traditional Renilla and Firefly luciferases (43, 44), as
277 the signal molecule for the assay. To create the assay components, RBD-binding nanobody
278 Ty1 (28) was fused with fragments of NanoLuc, titled SmBit or LgBit (42, 44), using flexible
279 (GGGGS)₄ linkers to connect the nanobody monomer and the signal molecule fragments
280 (Figure 5).

281 We performed proof-of-principle experiments to gauge the ability of the nanobody-
282 nanoluciferase fusions to detect recombinantly produced SARS-CoV-2 Spike in solution. 10
283 nM concentrations of each nanobody fusion, one fused to the LgBit and the other to the SmBit
284 fragment, were mixed with a dilution series of either recombinant spike or negative control
285 protein (BSA) and incubated for 15 minutes. The substrate of the nanoluciferase was added
286 immediately before measurement of luminescence from the reactions. The results show that
287 the spike signal can be distinguished from an equimolar concentration of the negative control
288 protein at a concentration as low as 200 pM (Figure 5).



289

290 **Figure 5. SARS-CoV-2 spike protein detection with a proximity-triggered assay.** A) Split
291 nanoluciferase fragments are fused to Ty1 nanobody (47) with GGGGS₄ linkers. The
292 enzymatic activity of the luciferase is restored upon nanobody binding to adjacent RBDs. B)
293 The reaction setup. The nanobody fusions are added into the wells of an opaque white plate
294 with recombinant spike, and the mixture is incubated for 15 minutes. Then, the substrate is
295 added, and the luminescence reads are recorded from each well. C) and D) The signal caused
296 by spike protein can be distinguished from background down to spike concentration of 200
297 pM.

298

299 Discussion

300 In this study, we created potent SARS-CoV-2 neutralizers and a diagnostic assay through
301 fusions of spike-targeted nanobody modules. Our multimodular nanobodies were linked
302 together with GGGGS₄-linkers to facilitate simultaneous binding of the modules to distinct
303 epitopes (Figure 1) and to increase the avidity of binding. We observed a notable increase (up
304 to 100-fold) in the neutralization potency of the multimodular constructs relative to the reported
305 IC₅₀ values of the single constituent nanobodies (SI Table S1) in neutralization assays
306 performed with SARS-CoV-2 wild-type, Alpha, and Delta variants of concern. Multimodular

307 nanobodies showed IC₅₀ values in the 50–160 pM range (Figure 3A-B) in cell culture, and, in
308 an animal model, prophylactic administration of tri-TMH in the nasal cavity limited tissue
309 damage in the lungs (Figure 3C).

310 SARS-CoV-2 variants have become the prevalent forms of the virus globally, which warrants
311 that the potency of new neutralizers is validated against these targets. While WT, Alpha, and
312 Delta variants were efficiently neutralized by multimodular nanobodies in this work, Beta and
313 Omicron were significantly less susceptible to neutralization (Figure 3), despite the capability
314 of tri-TMH and tri-TMV nanobodies to bind variant forms of the RBD (Figure 2). This agrees
315 with the previously noted pattern of potent antibodies lacking breadth in SARS-CoV-2
316 neutralization (65).

317 The MD simulations performed in this study indicate that the E484K amino acid change results
318 in a loss of salt bridge with conserved R52 and larger conformational rearrangement in the
319 receptor-binding domain (Figure 4), causing disruption of the nanobody binding interface and
320 leading to the Beta variant escaping neutralization. Notably, the MD simulation data also
321 revealed interaction trends at the antigen interface that correlate well with the experimentally
322 observed neutralization capacity (Figure 3). We postulate that this approach, focused on
323 simulating hydrogen bonding networks and RMSD trends at the antigen interface of emerging
324 variants may be applied to qualitatively predict the potential for escape from specific
325 neutralizers.

326 Drawing from the established field of protein-fragment complementation assays, we were
327 inspired to combine high-affinity nanobody modules with signal molecules to develop new
328 diagnostic tools. Our novel nanobody-based diagnostic assay was successful at detecting low
329 concentrations of SARS-CoV-2 spike protein. This is in line with the limit of detection reported
330 for other antigen test approaches, such as a FRET-based assay (66) and similar to the

331 commercially available rapid point-of-care antigen tests (40). To our knowledge, this is the
332 first report of a nanobody-based diagnostic approach that makes use of the protein-fragment
333 complementation toolkit. The observed level of detection shows potential for diagnostic use,
334 although future applications would require further validation of the technique with patient
335 samples. In contrast to monoclonal antibodies commonly used in diagnostics, engineered
336 nanobodies have multiple attractive properties, including cheap and scalable production that
337 does not require resource-intensive animal tissue cultures (51). It is also becoming feasible to
338 discover nanobodies from synthetic libraries, allowing the transition away from conventional
339 animal immunization prevalent in antibody generation (67). Established platforms for the
340 discovery of nanobodies will allow the application of the diagnostic assay presented here to
341 different targets, including viruses emerging in the future. We envision that this combination
342 of nanobody modules with split signal molecules presents a powerful platform for the rapid
343 development of single-step detection assays for emerging pathogens.

344 The COVID-19 pandemic continues, despite substantial efforts to curb the spread of the
345 disease, and emerging variants continue to pose challenges for potential SARS-CoV-2
346 therapeutics. Nanobodies, being inexpensive and readily modified, show great promise as viral
347 inhibitor candidates and diagnostic tools. Exploring the application of engineered nanobodies
348 against viral pathogens will facilitate the development of therapeutics against present and
349 future outbreaks of emerging infectious disease.

350

351 **Materials and Methods**

352 **Production and purification of multimodular and luciferase-fused nanobodies.** The
353 synthetic genes encoding multimodular nanobody constructs and nanobody fusions with split
354 nanoluciferase were obtained as inserts in pET100/D-TOPO vector backbones (GeneArt,

355 Thermo Fisher Scientific). Nanobodies were expressed in the bacterial cytoplasm using
356 *Escherichia coli* Rosetta-gami 2 (DE3) cells (Novagen) in autoinduction media. Expression
357 cultures were grown at 37 °C until OD600 reached 0.5, after which the incubation temperature
358 was lowered to 28 °C. The cells were harvested after 24 h from inoculation by centrifugation
359 at 4000 × g, 4 °C, for 15 min. The cell pellets were washed by resuspension in PBS. The pellets
360 were flash-frozen in liquid nitrogen and stored at -75 °C until purification.

361 To purify the nanobody constructs, the bacterial cell pellets were resuspended in lysis buffer
362 (10 mM Tris-HCl pH 7.5, 150 mM NaCl). Protease inhibitors and 10 mM imidazole were
363 added to the lysis buffer when purifying the tri-TMH and tri-TMV constructs. Cytoplasmic
364 proteins were extracted by lysing the cell suspension in Emulsiflex C3, and the lysate was
365 clarified by centrifugation at 38 000 × g for 30 min at 4 °C. The clarified lysate was loaded on
366 a HisTrap FF crude column and washed stepwise with lysis buffer containing 0, 10, 20, 30, and
367 50 mM imidazole, followed by elution with 300 mM imidazole. The eluate was concentrated
368 and buffer-exchanged into lysis buffer to remove imidazole using an Amicon Ultra 15 10K
369 concentrator.

370 To produce an ultrapure nanobody sample, the nanobodies were purified by size-exclusion
371 chromatography (SEC), using the ÄKTA Go system and a Superdex 75 Increase 10/300
372 column. When preparing samples for *in vivo* experiments, sample buffer was exchanged into
373 PBS during SEC. The pooled SEC fractions were further concentrated using an Amicon Ultra
374 10K 0.5 mL concentrator. Buffer-exchanges, when necessary, were performed in the same
375 device.

376 To prepare the nanobodies for neutralization assays, His-tags were removed from the proteins
377 by enterokinase cleavage (Bovine enterokinase, GenScript). Thereafter, the cleaved tags and

378 enzyme were removed from the sample using HisPur Ni-NTA resin (Thermo Scientific) or
379 SEC as described above.

380 **Production and purification of recombinant SARS-CoV-2 S protein.** SARS-CoV-2 spike
381 was expressed from a synthetic cDNA template (GeneArt, Life Technologies) encoding the S
382 protein ectodomain residues 14–1208 from the Wuhan-Hu-1 strain (NCBI Reference
383 Sequence: YP_009724390.1) stabilized in the prefusion state (4, 7) with proline substitutions
384 at residues 986 and 987, an abrogated furin S1/S2 cleavage site with a “GSAS” substitution at
385 residues 682–685, and a C-terminal T4 fibritin trimerization motif. In our construct, the
386 trimerization motif was followed by an HRV3C protease cleavage site, SpyTag003 (68), and
387 8xHisTag. The gene was cloned into the mammalian expression vector pHLsec (69) and
388 transfected into Expi293F™ (Thermo Fisher Scientific) suspension cells at a density of
389 3×10^6 cells per ml using the ExpiFectamine™ 293 Transfection Kit (Thermo Fisher
390 Scientific). Transfected cells were cultivated on an orbital shaker at 36.5 °C and 5% CO₂ for
391 six days, after which supernatant was harvested, clarified by centrifugation, filtered through a
392 0.45 µm filter, and supplemented with imidazole to 3 mM final concentration. SARS-CoV-2
393 S-protein was purified from the supernatant by immobilized nickel affinity chromatography
394 with a 1-ml HisTrap excel column (Cytiva) using 300 mM imidazole for elution. The eluate
395 was concentrated and buffer exchanged to 10 mM Tris pH 8 + 150 mM NaCl buffer using an
396 Amicon Ultra centrifugal filter (MWCO 100 kDa, Millipore). Pure S-trimer was used for cryo-
397 EM grid preparation immediately after purification.

398 **Cryo-EM grid preparation, data acquisition and data processing.** A 3-µl aliquot of a pure,
399 prefusion SARS-CoV-2 S-trimer (0.3 mg/ml) mixed with tri-TMH (0.05 mg/ml) was applied
400 on Quantifoil 1.2/1.3 grids (1.2-µm hole diameter, 200 mesh copper) that had been glow
401 discharged in Plasma Cleaner PDC-002-CE (Harrick Plasma) for 30 s. The grids were blotted

402 for 6 s and plunged into liquid ethane using a vitrification apparatus (Vitrobot, Thermo Fisher
403 Scientific).

404 Data were collected on a Titan Krios transmission electron microscope (Thermo Fisher
405 Scientific) equipped with Gatan K2 direct electron detector. EPU v 2.11.0 software was used
406 to acquire micrographs, and images were collected with a dose of $1.38 \text{ e}^-/\text{\AA}^2$ per image (SI
407 Table S2).

408 Data were processed in cryoSPARC (70) Movie frames were aligned and averaged to correct
409 for beam induced motion. Contrast transfer function (CTF) parameters were estimated using
410 CTFFIND4 (71). An initial set of particles, picked with the blob-picker, was classified and the
411 particles in good 2D classes were used to train Topaz particle picker (72, 73). A total of 91,601
412 particles were selected after cleaning the picked set with 2D classification. An initial volume
413 with C3 symmetry was calculated *ab initio*. A consensus map of the S trimer, with C3
414 symmetry applied, was resolved to 2.66-Å resolution. Visual inspection showed that the RBD
415 region was poorly defined in the consensus map. 3D variance analysis or symmetry-expanded
416 particles was run using a spherical mask defining the RBD region, six principal modes (i.e.
417 eigenvectors of the 3D covariance) and eight classes (or clusters). Particles in each class were
418 subjected to local asymmetric refinement (standard deviation over the prior of rotations and
419 shifts were 5 degrees and 5 Å, respectively, centered at the box center). This local refinement
420 prevented symmetry expanded particles from rotating over their symmetry copy. Particles in
421 the cluster corresponding to the “all-down” conformation were subjected to a second round of
422 3D variance analysis using 4 principal modes and 4 classes. Particles from 3 of the 4 classes
423 were combined, symmetry copies removed with the “remove duplicates” function and the map
424 was locally refined with C3 symmetry. Resolution of the maps was estimated based on the
425 gold-standard Fourier shell correlation (FSC) criterion of 0.143 (74), and the final maps were
426 filtered to local resolution.

427 Nanobodies were placed in the cryo-EM density maps by docking molecular models of the S
428 trimer (PDB: 7A29) and nanobody-RBD complexes (PDB: 6ZHD, 6ZXN, 7CAN) into the
429 map. First, the “fitmap” function of UCSF Chimera was used to simulate a density for the PDB
430 reference model to the global resolution of each map. The comparison of the simulated maps
431 with corresponding reconstructions by the “fitmap” function yielded correlation scores of
432 0.7269 for the 1-up map and 0.7367 for the all-down map. The “matchmaker” function in
433 UCSF Chimera was used to match models of nanobody-RBD complexes with the RBDs of the
434 full spike model. To account for the mobility of the RBDs, the individual Nb-RBD models
435 were further fitted into the density by the “fitmap” function (correlation scores for Nb-RBD
436 models: 1-up map 0.8064, 0.7843, 0.7824; all-down map 0.7937, 0.7799, 0.8017). This fitting
437 process resulted in nanobodies being placed into the remaining density regions unaccounted
438 for by the spike model.

439 **Proof-of-concept tests for the diagnostic assay with Split NanoLuc-nanobody fusions.** A
440 dilution series was made in triplicate with purified recombinant Spike in Tris buffer (10 mM
441 Tris-HCl pH 7.5, 150 mM NaCl). In each well, purified Ty1-LgBiT and Ty1-SmBiT constructs
442 were added at 10 nM final concentration each. In parallel, an equimolar dilution series of
443 bovine serum albumin was identically treated with the nanobody constructs to determine the
444 signal-to-noise ratio in the luminescence reaction. The mixture was incubated for 15 minutes
445 at room temperature, after which the nanoluciferase substrate coelenterazine H was mixed into
446 the sample at 200 nM final concentration. Immediately following substrate addition, the
447 luminescence readings were measured with Perkin-Elmer EnSpire multimode plate reader,
448 using the ‘Luminescence’ program. To calculate the final luminescence measurement while
449 taking noise into account, the average readings of each triplicate sample were divided with
450 corresponding averages from the BSA dilutions.

451 **Labelling of nanobodies with DyLight 633.** The nanobodies were labelled with DyLight 633
452 in PBS supplemented with 50 mM sodium borate (pH 8.5) at 1 mg/mL protein concentration
453 and 50 μ M Dylight 633 NHS ester (Thermo Fischer Scientific) at room temperature for 2h,
454 followed by removal of unreacted dye with Zeba Spin 7K MWCO desalting columns (Thermo
455 Scientific).

456 **Antigen array.** Wild type and variant SARS-CoV-2 RBD and Spike S1 domains were
457 biotinylated and arrayed as duplicate spots (0.1 ng per spot) in the wells of streptavidin-coated
458 microtitration plates using a piezoelectric non-contact microarray dispenser (Nano-Plotter,
459 GeSiM, Germany). The antigens were purchased from the following sources: RBD wt (aa 319-
460 541 of the S protein) and S1 wt (aa 14-681 of the S protein) from Medix Biochemica; RBD
461 single mutants K417N, E484K and N501Y and S1(K417N, E484K, N501Y, D614G)
462 quadruple mutant from SinoBiological.

463 **Binding assays on antigen array.** The antigen arrays in microplate wells were blocked with
464 50 μ L of Assay buffer (Tris-buffered saline (TBS), pH 8.0 + 0.05% Tween 20) per well for 30
465 min at RT, followed by three washes with Washing buffer (TBS containing 0.05% Tween 20).
466 DyLight 633 -labelled nanobody solutions (1 μ g/mL in Assay buffer) were added 50 μ L/well,
467 incubated in a plate shaker at 600 rpm, RT for 1h, followed by three washes with Washing
468 buffer. Residual liquid droplets were removed by centrifuging the plate upside down on a paper
469 towel in a plate adapter (453 g, 1 min), after which the plate was let dry for 15 min in a 37°C
470 room. The Dylight 633 -labelled nanobodies bound to the arrayed antigens were detected by
471 fluorescence scanning through the clear bottom of the microplate with a Tecan LS400 confocal
472 laser scanner, using a 633 nm laser for excitation and a 670/25 emission filter.

473 The fluorescence scan images were analyzed with Array-Pro Analyzer software (Media
474 Cybernetics) and the raw spot signal data was exported to Microsoft Excel for further

475 calculations. Net signals were obtained by subtracting the well background from the raw spot
476 signals (average pixel intensity in the spot area), after which the spot signals were normalized
477 to the wild type antigen spot signals in the same well: single RBD mutant signals were
478 expressed as percentage of the RBD wt signal whereas the quadruple S1 mutant signal was
479 expressed as percentage of the S1 wt signal.

480 **Neutralization assays.** VeroE6-TMPRSS2-H10 cells (66) were seeded to 96-well plates
481 (white-sided optically clear bottom PerkinElmer) in density 30 000 cells/well 24 h before the
482 assay. The nanobodies were diluted in series 1:150 000, 1:300 000, 1:600 000, 1:1 200 000,
483 1:1 240 000, and 1:4 800 000 in virus growth medium (VGM) containing MEM (Sigma, 2279),
484 2 % FBS, L-glutamine, and 1x penicillin-streptomycin. Diluted nanobodies were mixed with
485 the 50 pfu (Figure 3) or MOI 1 (SI Figure S5) (for wild-type, Alpha, Beta, and Delta) or MOI
486 0.2 (for Omicron) virus and incubated for 1 h at 37°C 5% CO₂. Thereafter, the cells were treated
487 with the mixture of the nanobodies and the virus. The virus dilution in VGM without the
488 nanobodies was used as a negative control and non-infected cells (MOCK) was used as a
489 positive control of the nanobody neutralization effectiveness. After 5 days of incubation the
490 medium was removed, and cells were treated with CellTiter-Glo 2.0 cell viability assay reagent
491 (Promega, G9243) for 20 min at RT. Then, the cellular ATP was measured via the detection of
492 luminescent signal using HIDEX Sence microplate reader (Hidex Oy, Finland) Viability of the
493 MOCK infected cells was considered as 100 %. Neutralization efficacy percentage for each
494 measurement was calculated considering MOCK infected cells as 100% neutralization and
495 untreated, virus infected cells as 0% neutralization. Curve-fitting and IC₅₀ calculation was
496 performed for the normalized neutralization data with GraphPad Prism version 9.2.0 for
497 Windows, using the Nonlinear regression method (Absolute IC₅₀, X is concentration), with
498 baseline constraint set to zero.

499 **Animal experiments.** A total of 20 male and female Syrian Golden hamsters were obtained
500 from (Scanbur, Karl SloaneStran, Denmark), moved to the University of Helsinki biosafety
501 level-3 (BSL-3) facility and allowed to acclimatize to individually ventilated biocontainment
502 cages (ISOcage; Scanbur, Karl SloaneStran, Denmark) for seven days with ad libitum water
503 and food (rodent pellets) prior to infection.

504 For the main experiment, six 8-week-old male and female Syrian Golden hamsters received 30
505 μg of nanobody, in 0.61 mg/mL concentration, 6 h prior to intranasal infection with 5×10^4
506 SARS-CoV-2 (wt/D614G strain). The control group received an equal volume of PBS (n = 4).
507 Euthanasia was performed under terminal isoflurane anaesthesia with cervical dislocation and
508 were dissected immediately after death. Samples were collected from the lungs for RT-qPCR
509 and the remaining lung tissue including trachea, heart, oesophagus and bronchial lymph nodes
510 were immersed in 10% buffered formalin. After 48 h, the tissue was transferred to and stored
511 in 70% ethanol until processing for histological and immunohistological examination.

512 **RT-qPCR.** RNA was extracted from lung samples using Trizol (Thermo Scientific) according
513 to the manufacturers' instructions. Isolated RNA was directly subjected to one-step RT-qPCR
514 analysis based on a previously described protocol for RdRp (75) and for E and subE genes (76)
515 with TaqMan fast virus 1-step master mix (Thermo Scientific) using AriaMx instrumentation
516 (Agilent, Santa Clara, CA, USA). The actin RT-qPCR used for normalization is described in
517 (77). Fold differences between samples were calculated by the comparative Ct method (78)
518 using the average of normalized Ct values from non-nanobody treated infected animal lung
519 tissues as reference.

520 **Histological, immunohistological and morphometrical analyses.** Three to five cross
521 sections were prepared from the fixed lung tissue and routinely paraffin wax embedded.
522 Consecutive sections (3-5 μm) were prepared and stained with hematoxylin eosin (HE) for

523 histological examination or subjected to immunohistological staining for SARS-CoV-2 antigen
524 expression, using a previously published staining protocol (79). For immunohistology, the
525 horseradish peroxidase method was applied. Rabbit anti-SARS-CoV nucleocapsid protein
526 (Rockland, 200-402-A50) served as the primary antibody, and DAB (EnVision FLEX DAB+
527 Chromogen in Substrate buffer; Agilent) for visualization of antibody binding. All incubations
528 took place in an autostainer (Dako). Sections were subsequently counterstained with
529 haematoxylin.

530 For morphometric analysis, the immunostained sections were scanned (NanoZoomer-XR
531 C12000; Hamamatsu, Hamamatsu City, Japan) and analysed using the software programme
532 Visiopharm (Visiopharm 2020.08.1.8403; Visiopharm, Hoersholm, Denmark) to quantify the
533 area of viral antigen expression in relation to the total area (= area occupied by lung
534 parenchyma) in the sections. This was used to compare the extent of viral antigen expression
535 in the lungs between untreated and treated animals. A first app was applied that outlined the
536 entire lung tissue as ROI (total area). For this a Decision Forest method was used and the
537 software was trained to detect the lung tissue section (total area). Once the lung section was
538 outlined as ROI the lumen of large bronchi and vessels was manually excluded from the ROI.
539 Subsequently, a second app with Decision Forest method was trained to detect viral antigen
540 expression (as brown DAB precipitate) within the ROI.

541 **Molecular dynamics simulations of nanobody-RBD interface.** MD simulations were
542 performed on the model systems constructed using the cryo-EM structure of nanobody
543 monomers and RBD (PDB 6ZXX, 7CAN, 6ZBP). During model system construction long
544 glycine linkers were removed. VMD psfgen tool (80) was employed to add missing hydrogen
545 atoms, make point mutations, and solvate the systems with TIP3P water and 0.1 M NaCl to
546 give a total system size of ca. 150,000 atoms. The force field for all components of the system
547 was CHARMM36 (81). GROMACS v20.3 (82) was used for all equilibration and production

548 simulations. First, the initial systems were minimized with restraints on heavy protein atoms
549 ($20,000 \text{ kJ mol}^{-1} \text{ nm}^{-2}$). Following convergence, a 100 ps NVT equilibration was performed
550 with the same restraints, followed by a 10 ns NPT with the restraints only on the protein
551 backbone atoms. All restraints were removed for the production runs, which employed the
552 LINCS algorithm (83) to achieve a 2 fs timestep and used the Nosé -Hoover thermostat (84,
553 85) to maintain 310 K temperature and the Parrinello-Rahman barostat (86) to maintain 1 atm
554 pressure. The electrostatic interactions were controlled by the particle mesh Ewald method (87)
555 with a 12 Å cutoff, while the van der Waals cutoff was also 12 Å, with a switching distance of
556 10 Å. Multiple independent simulation replicas were performed and trajectories were
557 visualized and analyzed using VMD (80) and Pymol (The PyMOL Molecular Graphics System,
558 Version 1.2r3pre, Schrödinger, LLC). **Table S3** lists system setups and their respective lengths.

559 **Molecular graphics.** Molecular graphics images were generated using PyMOL (The PyMOL
560 Molecular Graphics System, Version 2.4.0a0, Schrödinger, LLC), UCSF Chimera (88), and
561 UCSF ChimeraX (89).

562 **Protein interface analysis.** Residues comprising the epitopes of nanobody modules Ty1 (PDB
563 6ZXX), H11-H4 (PDB 6ZH9), MR17-K99Y (PDB 7CAN) and VHH V (PDB 7KN6) on
564 SARS-CoV-2 S were identified using the PDB ePISA server (90).

565

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580 **Competing interests statement.** The authors declare no competing interest.

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