Representational similarity learning reveals a graded multi-dimensional semantic space

in the human anterior temporal cortex

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Abstract

Neurocognitive models of semantic memory have proposed that the ventral anterior temporal

lobes (vATLs) encode a graded, distributed, and multidimensional semantic space—yet

neuroimaging studies seeking brain regions that encode semantic structure rarely identify these

areas. In simulations we show that this discrepancy may arise from a crucial mismatch between

theory and analysis approach. Utilizing an analysis recently formulated to investigate graded

multidimensional representations, *representational similarity learning* (RSL), we decoded

semantic structure from ECoG data collected from the vATL cortical surface while participants

named line drawings of common items. The results reveal a graded, multidimensional semantic

space encoded in neural activity across the vATL, which evolves over time and simultaneously

expresses both broad and finer-grained semantic structure amongst animate and inanimate

concepts. The work resolves the apparent discrepancy within the semantic cognition literature

and, more importantly, suggests a new approach to discovering representational structure in

neural data more generally.

Conflict of interest

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50   **Introduction**

If you encounter a wolf when walking home through a dark wood, your mind readily

accomplishes some remarkable feats: it anticipates the animal's likely behavior, perhaps slinking

closer toward you; it assigns the thing a name, which you might shout to alert others ("wolf!");

and it directs you to change your own plans, maybe running back down the path. These feats

arise from the human ability to discern conceptual structure—to realize that the wolf, despite its

resemblance to friendly dogs in town, is nevertheless a quite different sort of animal.

This ability to represent and exploit conceptual structure is central to human semantic

cognition. Such structure is *graded* in that similarities vary along a continuum: wolves are highly

similar to coyotes, partially similar to elk, and quite distinct from birch trees or canoes. It is also

multidimensional in that concepts vary along myriad independent components: wolves and dogs

are similar in their shapes, parts, movements, and phylogeny, but different in their behaviors,

habitats, and diets. To capture these properties of knowledge, computational approaches to

semantics often represent concepts with *vector spaces*: the meaning of a word or image is

expressed as a point in an n-dimensional space (or equivalently as an n-dimensional vector) such

that the proximity between points expresses the similarity in meaning between the denoted

concepts. Cognitive science and machine-learning offer many techniques for estimating semantic

vector spaces from natural language (Pereira et al., 2016), feature norms(McRae et al., 2005), or

similarity-judgments(Hebart et al., 2020), and these methods have provided a critical empirical

foundation for studying human conceptual knowledge.

The well-known "hub and spokes" view of semantic representation suggests that the

anterior temporal lobes (ATLs) encode a graded, multi-dimensional semantic vector space that

expresses conceptual similarity structure for all concepts, extracted across all input and output

modalities, and from our experiences of each concept across time (Jackson et al., 2021; Lambon

Ralph et al., 2017; Patterson et al., 2007). This proposal has been useful for understanding

patterns of semantic deficits arising from temporal lobe pathology in fronto-temporal dementia

(Acosta-Cabronero et al., 2011; Hodges & Patterson, 2007; Lambon Ralph, 2014; Lambon Ralph

et al., 2007; Rogers et al., 2004; Snowden et al., 1989), anterior temporal resection (Drane et al.,

2008; Lambon Ralph et al., 2009; Schapiro et al., 2013), and herpes viral encephalitis (Gainotti,

2018; Noppeney et al., 2007; Rogers et al., 2004); stimulation and evoked response direct

neurophysiological explorations; (Abel et al., 2015; Y. Chen et al., 2016; Shimotake et al.,

2015); the effects of transcranial magnetic stimulation in ATL and other parts of the cortical

semantic system (Binney et al., 2010; Binney & Lambon Ralph, 2015; Jefferies, 2013; Lambon

Ralph et al., 2009; Pobric et al., 2007, 2010); and a variety of behavioral phenomena in

developing and mature cognition (Chen et al., 2017; Jackson et al., 2021; Rogers & McClelland,

2004, 2014). Yet perhaps the most direct empirical test of the proposal—multivariate analysis of

functional brain imaging data while healthy participants perform a semantic task—has yielded

decidedly mixed results. Some studies report successful decoding of semantic structure from

ATL areas (Bruffaerts et al., 2013; Devereux et al., 2018; Fairhall & Caramazza, 2013; Martin et

al., 2018; Peelen & Caramazza, 2012), but several others have observed such structure in

posterior areas (Carota et al., 2017; Carota et al., 2021; Chao et al., 1999; Connolly et al., 2012;

Haxby et al., 2001; Kriegeskorte, Mur, Ruff, et al., 2008; Martin, 2007, 2016; Sha et al., 2015),

within a left-lateralized peri-sylvian network (Binder & Desai, 2011; Binder et al., 2009;

Devereux et al., 2013; Fairhall & Caramazza, 2013), or even across the entire cortex *except* the

ATL (Huth et al., 2016).

As noted in a recent review (Frisby et al., 2023), such heterogeneity is typical of the

broader literature on brain imaging and semantics, and may reflect widespread variation in the

analytic techniques used to seek neural signals that encode semantic structure. A great many

different multivariate techniques have arisen over the past decade, often producing quite

different and even contradictory findings across studies. Often published results do not explicitly

articulate the rationale for selecting a particular analytic method, the assumptions underlying the

method, or the patterns of signal the method can/cannot detect. Consequently, it can be difficult

to compare findings across studies, or to understand what conclusions are licensed by a given

positive or negative result.

This paper assesses whether the gap between the neuroimaging and other literatures vis-

à-vis the role of ATL in semantics is a consequence of such issues, focusing on one of the most

common analytic techniques employed in these studies: representational similarity analysis

(RSA). Specifically, we consider the possibility that RSA is not well-suited to finding _graded_

multidimensional structure of the kind the ATL is hypothesized to encode. This may seem

surprising, since RSA was developed specifically as a tool for finding cognitive similarity

structure in neuroimaging data (Kriegeskorte, Mur, & Bandettini, 2008)—yet, as we will

demonstrate, the reliance of the approach on correlation significantly limits the kinds of signal it

can detect.

Study 1 assesses how these limitations will influence discovery of neuro-semantic

representations by applying the approach to simulated neural data where the target signals are

known to encode elements of structure in a true semantic similarity matrix derived from feature-

listing data. The results reveal critical blind spots for RSA. Study 2 then introduces a different

approach to neural decoding, _representational similarity learning_ (RSL; Oswal et al., 2016),

motivated by explicit hypotheses about the nature of the neuro-semantic code. We show that

RSL can provide insights into neuro-semantic representation that RSA cannot by making explicit

which aspects of the target structure are being successfully decoded, and by operationalizing

hypotheses about the neurosemantic code directly within the decoding model. Study 3 extends

the RSL approach to the analysis of very large neural datasets by describing a neurally-motivated

form of model regularization before applying it to investigate graded multidimensional semantic

structure in ECoG data recorded from the surface of human vATL. A previous RSA analysis of

the same data failed to detect graded, multidimensional and cross-domain semantic structure (Y.

Chen et al., 2016); we empirically assess whether an analytic approach informed by an explicit

hypothesis about the neural code yields a different conclusion. The results resolve the

contradiction in the literature and suggest a new path for multivariate neural decoding more

generally.

130   **Simulation study 1: Evaluating RSA.**

131   Simulation 1 evaluated whether the results yielded by RSA reliably indicate whether a set of

132   neural measurements encode graded, multi-dimensional semantic similarity structure of the kind

133   typically sought in functional imaging studies. Though the general approach is well known, its

134   limitations may be less familiar, so we begin with a brief overview of the method and some of

135   the challenges it faces when seeking graded, multivariate structure.

136   RSA aims to find sets of neural features—voxels, electrodes, or other measurements of

neuro-physiological activity—whose responses to various cognitive events (e.g., the perception

of a stimulus) jointly encode an independently-measured target structure. Typically, the target

structure is a *representational similarity matrix* (RSM; sometimes called a representational

dissimilarity matrix or RDM) in which the rows and columns correspond to the different stimuli

in an experiment and the entries indicate the cognitive/representational similarities between

stimuli. For semantic representation, entries in the target RSM indicate similarity of meaning

amongst pairs of concepts as estimated from behavioral or corpus data. To determine if a set of

neural features (e.g., voxels, electrodes, EEG sources, etc.) encodes the target similarities, the

experimenter estimates the pattern of neural activity evoked by each stimulus and computes the

pairwise similarities between these to create a *neural similarity matrix* (NSM). Correlations

between the RSM and NSM are computed separately for each participant, and brain regions

where these are reliably greater than zero are interpreted as encoding the target structure.

This approach faces at least five challenges when used to find *graded*, *multidimensional*

structure in neural codes:

    151   1. *Discrete vs graded structure*: reliable correlations with a continuous-valued target

152   RSM can arise even if the neural response is discrete or categorical. Thus, a positive

153   result does not indicate that the neural response encodes *graded* structure even if such

154   structure is present in the target RSM.

155   2. *One-dimensionality*: the correlation between RSM and NSM is inherently one-

156   dimensional. Thus, a positive result cannot provide evidence of multidimensional

157   structure in the neural response.

158   3. *A priori feature selection*: neural feature selection must be independent of and prior to

159   the representational analysis. Thus, a negative result may only imply that the feature

160   selection technique (e.g., ROI or searchlight) excluded signal carrying features.

161   4. *Equal importance*: all selected neural features are equally weighted when computing

162   the NSM. If the informative neural features are sparse or vary in signal strength, the

true signal may be overwhelmed by noise. Thus, a negative result does not indicate

that the selected neural features carry no target information.

5. *Masked dimensionality*: reliable correlations between RSM and NSM can be driven

by a subset of the RSM structure or items. Thus, a positive result does not imply that

the entire target RSM is encoded.

Simulation 1 assessed how these characteristics of RSA will influence discovery of

neuro-semantic representations by applying the approach to simulated neural data encoding

different aspects of a real semantic similarity matrix.

Methods

The target RSM was computed from semantic feature norms for 100 items, half animate

and half inanimate, collected in prior work (Dilkina & Lambon Ralph, 2013). The feature vectors

for each item were aggregated in a matrix with rows indicating words, columns indicating

features, and binary entries indicating whether the referent of the word possesses that feature.

Matrix columns were mean-centered and the RSM was computed as the cosine similarity for all

pairs of row vectors.

To understand the latent structure of the RSM, we used singular value decomposition

(SVD) to extract three components accounting for 90% of the variance in the full matrix.

Figure 1 shows the coordinates for all 100 items on each latent dimension, color coded by

semantic category (see Appendix A for full list of items and how they were categorized). The

decomposition reveals graded semantic structure along each dimension. The first separates

animate from inanimate items but also individuates subcategories in each domain. The second

strongly differentiates subcategories of animals but also weakly distinguishes inanimate

subcategories. The third differentiates the inanimate items, though the resulting spread is less

Figure 1. Coordinates of the 100 stimuli in the three-dimensional singular-value-decomposition of the semantic similarity matrix. Colors show category membership within each domain. Component 1 separates animate from inanimate items, but also separates animate sub-categories. Component 2 largely separates animate sub-categories, while component 3 largely separates inanimate sub-categories.

"clumpy" than within animate items as commonly found with such data (Lambon Ralph et al.,

2007).

The simulation assessed what results RSA would yield when applied to a neural signal

known to encode elements of this underlying semantic structure. Specifically, we created five

simulated neural datasets, each capturing a different aspect of semantic structure in the target

RSM. For each dataset we simulated the responses of 24 hypothesized neural features (e.g., the

BOLD response over 24 voxels in an ROI, or the mean evoked response at each of 24 electrodes)

to the 100 stimuli. Half of the simulated neural features encoded true semantic information about

the target items while half adopted random values sampled from a uniform distribution in the

same range. The five datasets varied in which aspects of the target matrix they encoded, as

illustrated in the schematic plots in **Figure 2A.** In the *binary condition*, all signal-carrying neural

features adopted one state (-1 or 1) for animate items and the opposite state for inanimate

items—thus the code was both one-dimensional and discrete. In three *one-D conditions*, all

signal-carrying neural features only encoded a single latent component of the target RSM—

either the first, second, or third singular vector as shown in **Figure 1**. Thus, each encoded *graded*

similarity structure but only *one* dimension of variation. In the *full structure condition,* the

signal-carrying units jointly encoded all three latent components of variation in the target

RMS—thus the code was both graded and multidimensional.

For each signal condition, we distorted the simulated neural responses to each stimulus

with measurement noise sampled from a uniform distribution centered on 0, generated a

simulated NSM, then computed the correlation between the simulated NSM and target semantic

RSM. This procedure was conducted 20 times at each of 11 increasing noise levels. We then

computed, across runs at each noise level, the mean and 95% confidence intervals of the Pearson

correlation between simulated NSM and RSM.

Results

The results are shown in **Figure 2B.** The binary code showed robust correlations across

the full noise-spectrum, illustrating that RSA can yield a positive result even when the neural

code is neither continuous nor multidimensional. Amongst the one-D codes, RSA showed a

strong positive result if the simulated neural response encoded the first singular vector of the

target matrix, but much weaker results that decayed to zero with increasing noise when the

neural response encoded other components. Thus, RSA can yield null results even when the

neural features under consideration *do* reliably encode semantic information that is orthogonal to

Figure 2. Simulation results. A. Each plot illustrates different ways that a neural response might encode some aspects of a target RSM, schematized in the rightmost plot ("All"). Vertical bars show the hypothesized responses of neural features to various animate and inanimate stimuli (red more active; blue less active; gray random) while the squares show the neural similarity matrices that would then result (red high similarity, blue low). All conditions encode some components of the full RSM and so should be detected by a multivariate method seeking semantic structure. B. Curves showing the expected results of standard RSA when used to decode real semantic structure from the target RSM under different hypotheses about the neural code and increasing amounts of measurement noise. Dots show the mean correlation while ribbons show the 95% confidence interval. The approach can yield robust results when the neural signal is discrete and/or one-dimensional, even under substantial noise, and can yield weak or null results when the neural signal faithfully encodes weaker components of the RSM, even under low-noise conditions. C. Results of RSL applied to the same simulated data, showing the correlation between true and predicted coordinates for held-out items on each latent component of the target matrix (columns), for the five different simulation conditions (rows), and computed across all items (black lines), animate items (red), or inanimate items (green). RSL shows a positive result in each case, identifies which components of the matrix are present in the neural code, and reveals reliable within-domain decoding only when the neural code expresses continuous similarity structure.

the primary component of the RSM. A strong correlation was observed when the neural features

encoded all three components of the target matrix and there was little noise in the signal, but this

declined steeply with noise. In high noise conditions, RSA yielded a more reliable result when

the simulated neural response encoded a binary domain distinction or just the first component of

variation. For these scenarios, all signal-carrying features encode the same information, so noise

"cancels out" across features and the signal remains robust. When the same number of features

encode three orthogonal components, fewer resources are dedicated to each, and corruption from

noise more seriously degrades the signal.

Discussion

The simulation shows that, when decoding semantic similarity structure of the kind

captured by semantic feature norms, RSA can yield a positive result when the neural response is

discrete and/or one-dimensional, and a null result when the neural response *does* encode

underlying dimensions of the target matrix beyond the strongest. Thus RSA, as typically

deployed, does not reliably indicate whether a set of neural signals encode the graded,

multidimensional semantic structure existing in a target RSM.

This result importantly constrains the conclusions that can be drawn from both positive

and negative results in the literature. For instance, consider the interesting findings of Clarke and

Tyler (2014), who used RSA to seek areas encoding semantic structure both across and within

superordinate domains (such as "animals" and "vehicles"). When the target matrix included all

items from all domains, the analysis identified the vATL as encoding semantic structure. When

limited only to items within one semantic domain, however, the vATL did not appear to encode

such structure. The finding could mean that vATL only encodes discrete distinctions between

superordinate semantic domains, analogous to the binary condition in the simulation—but the

same result could also obtain even if the vATL does encode within-domain structure, since such

structure is mainly encoded, within the semantic target matrix, by components orthogonal to the

primary dimension. Adjudicating these possibilities requires a method that can detect lower-rank

components of the target matrix.

245   **Simulation study 2: Decoding with RSL.**

246   These issues led us to consider an alternative approach designed explicitly to decode

graded, multidimensional similarity structure, called *representational similarity learning* (RSL;

Oswal et al., 2016). Rather than using pairwise similarities in the RSM as the target values for

decoding, RSL first decomposes the matrix into orthogonal latent components, effectively re-

representing each stimulus item as a point in a low-dimensional semantic space as shown in

Figure 1. It then uses linear regression to fit *decoding models* that predict the coordinates of each

item along each dimension from their evoked neural responses. Simulation 2 assessed whether

this approach can reveal the graded and/or multidimensional structure obscured by RSA.

Methods

255   Using the same simulated neural signals from Simulation 1 as predictors, we fit

regression models to predict coordinates of each stimulus along each of the three latent semantic

dimensions shown in **Figure 1**. For each simulated neural structure and each of 11 increasing

levels of uniformly-distributed noise, each example was assigned to one of ten mutually

exclusive test sets. Holding out each test set in turn, regression models were fit to the remaining

90% of the examples (the training set). The model that was fit to the training set predicts

coordinates for the 10% of examples withheld as the test set. After iterating over the ten test sets,

a hold-out prediction exists for every item. These were concatenated and correlated with the

target embedding one dimension at a time. This process was repeated 20 times with different

samples of noise. Hold-out accuracy for each condition and noise level was estimated as the

mean over simulation repetitions.

266   Multidimensional structure in the neural code should be revealed by reliable prediction of

coordinates along more the one latent dimension. To assess whether the neural code captures

graded similarity, we evaluated how well the fitted model predicted coordinates amongst just the

animate items or just the inanimate items. If the neural signal only categorically differentiates

animate from inanimate stimuli, then predicted and true values should correlate significantly

when models are evaluated on all items but should *not* correlate amongst just the animate or just

the inanimate items considered separately. Reliable intra- and inter-domain correlations between

true and predicted values thus indicate that the neural code captures a graded degree of similarity

structure.

Results

Figure 2C shows the mean correlation between true and predicted coordinates for held-

out items on each of the three target components (columns), for the five different neural coding

scenarios (rows), and computed across all items (black lines), animate items (red), or inanimate

items (green). The pattern of results reveals the information encoded in each simulated neural

response. With the binary neural signal (top row), predicted and true coordinates correlated

strongly for models fit to all items but not separately for animates vs inanimates. With

continuous one-D signals, strong correlations were observed for models fit to all items and

within each domain separately, but only for the dimension encoded by the neural response. When

the neural signal encoded graded multidimensional structure, reliable correlations were observed

on all three latent components, for models fit to all items and fit separately to each domain. Thus,

in simulation, the pattern of results uniquely revealed whether the neural signal encodes graded

or discrete structure, and which semantic dimensions it captures.

Discussion

In contrast to the RSA simulation, RSL yielded a different, diagnostic pattern of results

for each condition, indicating which aspects of the semantic target matrix were encoded within

the simulated neural responses. The discreteness of the binary code was revealed by reliable

prediction across domains and no reliable prediction within domain. In the 1D neural-structure

conditions, RSL showed reliable prediction only on the latent dimensions encoded by the

simulated neural signal, and not on the other dimensions. Reliable decoding both within and

between domains in such conditions indicated, in contrast to the binary condition, that the signal

is graded rather than discrete. When the simulated neural signal encoded all three semantic

dimensions, RSL showed reliable decoding of each. Thus, by considering decoding accuracy on

orthogonal components of the target matrix, RSL can test whether the neural code expresses

multidimensional structure; and by considering decoding accuracy separately for different

semantic domains, it can test whether the code is graded.

Study 3: Decoding semantic structure from ECoG using RSL

Study 3 evaluated whether neural signals in vATL encode a graded, multi-dimensional

and domain-general semantic space by using RSL to decode semantic structure in ECoG data

collected in a prior study of object naming (which employed the same 100 items used in the

simulations; Y. Chen et al., 2016). This dataset is especially useful in the current context for two

reasons.

First, ECoG avoids some of the limitations of non-invasive imaging methods that can

make structure in vATL difficult to decode. One recent study suggested that the neuro-semantic

code for animacy in vATL changes rapidly and nonlinearly over the course of stimulus

processing so that techniques sacrificing either spatial or temporal resolution, including EEG,

MEG, and fMRI, may obscure important signal (Rogers et al., 2021). Additionally, magnetic

field inhomogeneities make it difficult to resolve clear BOLD signal in vATL without special

acquisition sequences (Halai et al., 2015; Halai et al., 2014). ECoG provides unparalleled spatial

and temporal resolution of neurophysiological signals at the surface of cortex and does not suffer

from the signal-detection issues that challenge fMRI, so any failure to discover fine-grained /

multivariate semantic structure in the data cannot reflect these limitations.

Second, the results of the original RSA study (Y. Chen et al., 2016) suggest that the

measured signals, though reliably differentiating animate from inanimate items, do *not* encode

finer-grained or multidimensional semantic structure. Specifically, the authors compared the

correlation of the stimulus-evoked NSM to two different target matrices: one encoding the full

graded and multi-dimensional semantic similarities amongst stimuli, and a second encoding just

the binary distinction between animate vs inanimate items. If the vATLs encode graded multi-

dimensional semantic structure, one might expect the NSM to correlate more strongly with the

full target matrix than with the binary animacy matrix. Instead, the authors found statistically

significant and *equally strong* correlations with both target matrices. One interpretation of this

finding is that the measured neural signals do *not* in fact encode graded or multi-dimensional

semantic structure, but only serve to discretely differentiate animate and inanimate items—a

conclusion also consistent with Clarke & Tyler's (2014) RSA results described earlier. The data

thus allow us to test an alternative hypothesis: that the measured signals *do* encode a graded,

multi-dimensional and domain-general semantic space, in a manner that is invisible to RSA. If

so, RSL should reliably decode variation along multiple orthogonal components of the target

semantic matrix, considering all items together as well as within animate and inanimate domains

considered separately.

Applying RSL to ECoG or any other brain imaging data, however, faces an immediate

challenge: such technologies produce many more neural measurements than there are stimuli, so

regression models predicting stimulus characteristics from neural data are ill-defined (i.e., there

exist infinite solutions that can perfectly predict outcomes on training data even from random

input data). To find a unique fit without a priori feature selection, the regression must be

regularized to satisfy some additional constraint that will guarantee a single unique solution for

model fitting. For instance, the weight optimization might jointly minimize prediction error and

the size of the model coefficients, measured as the sum of their absolute values (the *L1-norm*).

Since this sum can be minimized by placing zero coefficients on many predictors, this form of

regularization promotes a sparse solution in which only a few predictors have non-zero

coefficients in the final model (e.g., Rogers et al., 2021). Other regularizers (such as the L2 norm

or the elastic net) enforce different constraints on model fitting, and thus lead to other solutions

when applied to the same dataset (Cox & Rogers, 2021).

347   In this sense, the selection of a regularization function amounts to a prior hypothesis

348   stipulating how the neural signal is likely to be structured. As recently argued in (Frisby et al.,

349   2023), the choice of regularizer should be informed by explicit hypotheses about the nature of

350   the signal to be decoded—in this case, a hypothesis about how neurophysiological signals

351   measured by surface electrodes in the brain might encode a graded, multi-variate semantic space.

352   To that end, we adopted a regularization function called the *group-ordered-weighted*

LASSO (grOWL) loss (Oswal et al., 2016) that was designed in prior work to capture three

theoretically-motivated assumptions about the structure of neural representations. First, it

assumes the signal is *sparse*: of all measurements taken, only a relatively small proportion

encode target information of interest, so the regularizer should place zero coefficients on many

predictors (as with L1 regularization). Second, it assumes *redundancy* in the true signal: neural

populations that do encode target information will be correlated in their activity patterns over

items, so the regularizer should spread similar coefficients across correlated signal-carrying

populations (similar to L2 regularization). Third, it assumes that signal-carrying populations are

unlikely to be "axis-aligned" with the target semantic space (i.e., responding only to variation

along a single semantic dimension) but more likely encode multiple, varying "directions" within

the space. That is, each neural population likely carries information about an item's coordinates

along multiple dimensions of the target space. We will refer to this as the *spanning* assumption,

since the selected neural features span the target representational space but are unlikely to only

encode distinct, individual dimensions. To enforce this assumption, the regularizer should prefer

solutions where coefficients on a given neural feature are either all zero (the feature does not

carry any information) or all non-zero (it predicts some variation along all target dimensions).

Oswal et al. (2016) showed that all three assumptions can be captured in a single convex

loss function, and also provided analytic guarantees and an example application on an fMRI

dataset. We describe the logic briefly here; Appendix B provides a formal description of the

decoding model and grOWL regularizer, including a definition of the loss and explanation of

how it encourages these properties in the decoding matrix.

Rather than fitting a separate regression model for each latent component of the target

RSM (as in the simulation), we instead predict all latent components (Figure 3A) simultaneously

by estimating the parameters of a *decoding matrix* β (Figure 3C). Suppose the coordinates of n

stimuli on r latent semantic dimensions are stored in matrix $U_{n \times r}$ while the responses of m

neural features to the stimuli are stored in matrix $X_{n \times m}$. RSL models the entries in U as the

matrix product of the neural activations in X and the decoding matrix $\beta_{m \times r}$: $U = X\beta$. Each row

of β corresponds to one neural feature (voxel, electrode, etc.), and each column encodes weights

for each neural feature when predicting stimulus coordinates on the corresponding dimension of

the target matrix U. Thus, the assumptions about neural signal just listed can be formalized

Figure 3. Representational similarity learning. A. To generate the target structure for decoding, semantic feature vectors for each of n items are mean-centered and converted to a cosine similarity matrix $\mathbf{S}_{n \times n}$ of approximate rank r. This is decomposed into matrix $\mathbf{U}_{n \times r}$ containing r orthogonal singular vectors and diagonal matrix $\mathbf{D}_{r \times r}$ containing singular values for each vector. The product $\mathbf{U}\sqrt{\mathbf{D}}$ is an nxr matrix whose columns contain r root-weighted singular vectors that are the target of the decoding model. Note that the product of this matrix with its transpose provides an estimate of the original matrix $\mathbf{S}_{n \times n}$. B. Neural responses in a picture-naming task are recorded for each stimulus as intra-cranial voltage potentials collected at 1000Hz over electrodes implanted in vATL. Data are concatenated across electrodes to create a single m-dimensional "neural feature vector" for each stimulus, where m is the total number of electrodes times the size of the decoding window in milliseconds. All such vectors are compiled into a neural feature matrix $\mathbf{X}_{n \times m}$ which contains the predictors for the decoding model. C. The target structure $\boldsymbol{U}\sqrt{\boldsymbol{D}}$ is then modeled as the product of the neural feature matrix $\boldsymbol{X}$ and a decoding matrix of regression coefficients $\boldsymbol{\beta}$ whose values are chosen via gradient descent to minimize prediction error plus the regularization penalty $H(\boldsymbol{\beta})$ scaled by the weighting parameter α. D. Definition of the group-ordered-weighted LASSO (grOWL) regularization function and illustration of the structure it promotes in the decoding matrix.

383   as constraints on the structure of the decoding matrix $\boldsymbol{\beta}$ (**Figure 3D**). To capture the sparsity and

384   spanning assumptions, $\boldsymbol{\beta}$ is constrained to be *row-sparse*: most rows have all zero values

385   (sparsity), and the rest have all non-zero values (spanning). To capture the redundancy

386   assumption, highly correlated and signal-carrying neural features receive similar row-vectors in

387    $\boldsymbol{\beta}$ (**Figure 3D**). **Figure 3** shows the full workflow decoding semantic structure from ECoG data.

388   With this overview we can consider how RSL can be applied to assess whether neural

data encode a multidimensional and graded similarity space. Parameters in $\boldsymbol{\beta}$ are estimated for a

batch of training data using regression regularized with the grOWL loss. The decoding model is

then applied to predict the coordinates of held-out items along each dimension in the target

representation space. If predicted and true coordinates for held-out items correlate reliably on

more than one dimension, the neural signal must encode multidimensional structure. To assess

whether the neural code captures graded similarity, we additionally evaluate the regression

models separately for animate and inanimate items, as in the simulation. If the neural signal only

categorically differentiates animate from inanimate stimuli as suggested by the prior RSA

analysis in Y. Chen et al. (2016), then predicted and true values should correlate significantly

across all items, but not for animate or inanimate subsets considered separately. Observation of

both inter- and intra-domain correlations thus indicates that the neural code captures a graded

degree of similarity structure. Finally, to assess how well the decoder recovers the target

semantic similarities, the predicted coordinates for held-out items on all three latent dimensions

can be used to estimate semantic distances between stimulus pairs. These estimates can then be

correlated with true semantic distances, similar to standard RSA.

Methods

We applied this approach to the same ECoG dataset where prior work using RSA found

no evidence for graded multidimensional structure (Y. Chen et al., 2016). The study was

approved by the ethics committee of the Kyoto University Graduate School of Medicine (No.

C533) and participants provided written informed consent. The dataset contains voltages

measured from platinum subdural grid electrodes (inter-electrode distance 1 cm and recording

diameter 2.3mm; Ad-Tech, WI) implanted in the surface of left (8) or right (2) vATL in ten

patients undergoing preparation for intractable epilepsy (9) or brain tumor (1) while they named

line drawings depicting the 100 items described in Study 1. Electrodes were implanted in the

right hemisphere if language was not left-lateralized as determined by the WADA test.

Each patient had between 6 and 32 electrodes (mean of 20) covering vATL. All patients

with epilepsy had seizure onset zones outside the anterior fusiform region, except one patient for

whom it was not possible to localize the core seizure onset region. Data were sampled at 1000Hz

(eight patients) or 2000Hz (two patients) with a band-pass filter of 0.016 – 300 (eight patients) or

0.016 – 600Hz (two patients). The dataset included, for each stimulus, voltages measured at each

electrode over a 1s window from stimulus onset and downsampled to 100Hz. Thus, for a

participant with 20 electrodes, each stimulus was associated with a 2,000-element vector of

voltages (20 electrodes x 100 time points).

Stimuli and Procedure

One hundred line-drawings (50 animate and 50 inanimate items) were obtained from

previous norming studies (Morrison et al., 1997; Snodgrass & Vanderwart, 1980). See Y. Chen

et al. (2016) for a complete list. Animate and inanimate stimuli were matched on age of

acquisition, visual complexity, familiarity, and word frequency, and had high name agreement.

Each stimulus was presented on a computer screen for 5 seconds, one after another with no

interstimulus interval, once during each of four sessions (four times in total). Each session

proceeded in a different random order. Participants were instructed to name each item as quickly

and accurately as possible. Participants were video and audio recorded during the experiment.

Video was used to monitor eye fixations and general attention to the task. The mean response

latency was 1190ms.

Semantic similarity structure and dimensionality reduction.

The same target RSM and 3-dimensional embedding used in the simulated analysis are

reused for the ECoG analysis.

ECoG data preprocessing. Preprocessing was performed in MATLAB. Data were

downsampled to 100Hz by averaging measurements within 10ms boxcars. A prior study

applying pattern classification to these data found near identical results when analyzing raw

voltages versus voltages referenced to the electrode beneath the galea aponeurotica or to the

scalp electrode on the mastoid process contralateral to the side of electrode implantation (Rogers

et al., 2021). For this reason, and because the location of the reference electrode varied across

patients, we analyzed all voltages without referencing. For each stimulus we retained data for

1000ms from stimulus onset. While the trial epoch may include the onset of articulation toward

the end, the critical results cannot reflect such motor activity since all key phenomena are

observed early in the epoch. Baseline correction was not performed. The mean voltage at each

electrode for each stimulus was computed across the four repetitions. Voltages from different

electrodes were concatenated into a row vector and arranged in a neural data matrix with each

row containing the vector of voltages for one stimulus sampled from multiple electrodes over

time. We rejected columns and then rows where the marginal mean was more than five standard

deviations from the grand mean to censor extreme outliers.

Model fitting and evaluation

RSL decoding models regularized with either grOWL or the L1-norm were fit and

analyzed in MATLAB v9.5 (MathWorks, 2018) using the Whole-brain Imaging with Sparse

Correlations (WISC) toolbox (Cox, 2021), which implements the approach as a multitask variant

of group ordered weighted L1-regularized regression (grOWL; Oswal et al., 2016; Oswal &

Nowak, 2018).

Fitting a decoding model regularized with grOWL requires two hyper-parameters that

govern pressured the strength with which the decoding matrix is to be row-sparse (λ) with

similar weights across correlated neural features (ω). We chose values for λ and ω via ten-fold

nested cross-validation for each model fit. The 100 stimuli were randomly divided into ten

subsets, each containing five animate and five inanimate items. On each of the ten folds, one of

the ten subsets was held out (outer-loop holdout). The remaining nine sets were used to search

for good hyperparameter values, involving a second "inner" cross-validation loop.

On each inner-loop fold, one of the nine remaining sets was held out and a decoding

model was fit to the remaining eight sets using a specified pair of hyper-parameter values. The

fitted model's prediction error, defined as the Frobenius norm of true versus predicted semantic

coordinates, was evaluated on the inner-loop holdout set. This procedure was repeated once for

each of the nine inner-loop holdouts before averaging the prediction error across folds to

estimate the decoder's performance with that hyperparameter configuration. Many different

hyperparameter configurations were evaluated in the inner loop using the Hyperband procedure

(Li et al., 2018). The best-performing configuration was then used to fit a model to all examples

not in the outer-loop holdout set. This tuned model was used to predict semantic coordinates for

the outer-loop holdout set, thus completing one iteration of outer-loop cross-validation. The

whole procedure was then repeated for the remaining nine outer-loop holdout sets. Across folds,

the procedure generated out-of-sample predicted coordinates for all 100 items. These final

predicted coordinates, computed separately for each time-window in each participant, were the

primary data evaluated in the results.

Statistical thresholding with permutation testing

Our analyses closely followed the simulations: correlations between predicted and true

coordinates on each dimension were computed for all 100 stimuli, just the 50 animate items, or

just the 50 inanimate items. Assessing model accuracy via correlation standardizes means and

variances of the target and predicted vectors to focus on just their covariance. This is especially

critical when evaluating animate and inanimate items separately. However, cross-validated

correlation has a negative bias when evaluating held-out items (see Zhou et al., 2017 and

Appendix C); a null hypothesis of zero with a t-distributed sampling distribution cannot be

assumed. Thus, we determined statistical reliability at the group level by constructing an

empirical null distribution via a permutation procedure described by Stelzer et al. (2013). The

analysis described above was repeated 100 times per participant, each time with a different

random permutation applied to the rows of the target matrix. This yielded 100 correlation values

for each patient, representing expected values from our workflow when no reliable relationship

exists between neural data and target matrix (due to the permutation procedure). Then, a group-

level empirical null distribution was estimated by randomly sampling one of the 100

performance metrics from each participant-level distribution and computing a permuted-group-

average 10,000 times. This provided sufficient resolution at the group level at a fraction of the

computational cost of fitting models to 10,000 permutations of the target matrix per participant

for each test (i.e., each window, for each subset of items, in all analyses).

If m is the number of values in the permutation distribution and b is the number of values

in the distribution larger than the true correlation value, then the one-tailed p-value can be

computed (Edgington & Onghena, 2007; Phipson & Smyth, 2010) as:

500
$$p = \frac{b + 1}{m + 1}$$

Statistical significance was defined with respect to $\alpha < .05$ after adjusting the p-values to

control the false discovery rate (FDR).

Finally, to understand the effects of regularization with structured sparsity (grOWL) vs.

more standard techniques, we compared models fit with grOWL regularization to those fit with

L1 (LASSO) regularization.

Results

Analysis 1: Full window decoding with grOWL and LASSO

Figure 4a shows results from decoding the full 1000-ms time-window. For the first

component, models fit with both grOWL and LASSO reliably decoded similarity structure across

all items and for animate and inanimate subsets considered separately. Whereas this was the only

structure discovered with LASSO regularization, grOWL regularization additionally showed

reliable decoding of the second component across all items and within animates only. Thus, RSL

with grOWL regularization revealed graded, multidimensional semantic structure in ECoG

signals recorded from ventral ATL, while the contrasting pattern for LASSO suggests that

additional constraints from grOWL aided in the discovery of multidimensional semantic

structure.

Figure 4. ECoG decoding results. Correlation between true and predicted coordinates along each latent dimension (columns) for models fit to all items (green), animate items only (orange), or inanimate items only (blue), and regularized with grOWL or LASSO. Error bars reflect standard error of the mean over participants. Each value is centered on the mean of its corresponding permutation distribution. For uncentered values, see Figure S4. Colored bars / filled circles indicate reliable decoding with FDR-corrected p < .05 for all points in a panel. a) grOWL and LASSO model performance when trained on the full 1000-ms trial epoch. b) grOWL model performance within opening windows. c) LASSO model performance within opening windows. d) Analogous to (b) except that models are fit and evaluated within a 100ms moving window instead of the opening window.

Analysis 2: Opening window

To see how this structure emerges in the ECoG signal over time, we conducted an "opening

window" analysis in which the same procedure was applied to an increasingly wide aperture of

data, beginning with just the first 50ms post-stimulus, extending to 100ms, then growing by

100ms up to 1000ms. The opening window analysis evaluates when enough information has

entered the spatiotemporal feature space to support decoding. The goal is not to localize a

representation in time, but to identify when reliable decoding is first possible and when

performance stops improving.

The results show reliable decoding of between-domain and within-animate structure

along the first component by 200ms, followed by within-inanimate structure by 300ms (Figure

4b). Decoding accuracy for superordinate and animate-subordinate structure continually

improved with wider windows along component 1, but not inanimate-subordinate structure.

Along the second component, reliable decoding was observed after 300ms for between-domain

structure and somewhat earlier (200ms) for within-animate structure. Within-inanimate structure

could not be reliably decoded along the second component at any window-size, nor could

variation along the third component of the target matrix. Models fit with LASSO (Figure 4c) also

reliably decoded both within- and across-domain structure along the first component, beginning

at 200ms for cross-domain structure, 300ms for a within-animate structure, and 500ms for

within-inanimate structure, but as with the full window, did not reliably decode the second (or

third) component for any window size.

Analysis 3: Moving window

The opening window analysis indicates the latency with which the neural signal contains

sufficient information for reliable decoding, but since each successive window contains all prior

time points, it does not indicate whether/how the neural encoding of semantic information

changes over time. Additionally, since larger windows contain more neural features, they afford

a greater possibility of over-fitting training data. Consequently, the opening-window approach

may fail to detect semantic information encoded only within a limited time-window. For these

reasons, we fit models using the grOWL regularizer on a 100ms *moving* window, beginning at

0ms from stimulus onset and advancing in 50ms increments. In this analysis, each window is the

same size and thus contains the same amount of neural data. Otherwise, the analysis was

identical to the opening-window variant.

Results are shown in Figure 4d. For component 1, reliable decoding was observed across

domains and within each domain between 150 – 700ms post stimulus onset. Reliable decoding

on components 2 and 3 was observed within a more limited time range. For component 2 (which

best-separates the animate items), cross-domain and within-animate structure was reliably and

equally-well decoded for windows beginning at 150 – 400ms. For component 3 (which best

separates inanimate items), cross-domain and within-inanimate structure was reliably and

equally-well decoded for windows beginning at 200 – 300ms. Together the analyses suggest that,

from around 200 – 400ms post-stimulus, neural states measured by ECoG express both within-

and between- domain semantic structure, for both animate and inanimate items, across all three

components of the target matrix. That is, they express a graded multi-dimensional and domain-

general semantic space.

Analysis 4: Moving-window reconstruction of full target similarity matrix

The preceding analyses consider decoding of each matrix component separately, allowing

us to draw conclusions about which aspects of semantic structure are represented in the neural

signal at which time points. The independent consideration of different dimensions, however,

makes it difficult to compare results of RSL to RSA, since RSA considers correlations between

full pairwise similarity matrices (the NSM and the RSM). To facilitate the comparison, we used

the decoding models fit in Analysis 3 to construct a *predicted semantic similarity matrix* at each

time-window. For each fitted model, we predicted coordinates of the corresponding held-out

items along all three target matrix components, agglomerating these predictions across hold-out

sets to create a matrix of predicted coordinates for all items. Recall that the target coordinates are

the first three singular vectors of the original semantic similarity matrix, weighted by the *square*

root of the corresponding singular values (**Figure 3**). Thus, to reconstruct predicted pairwise

distances in the original target matrix, we need only take the product of the predicted-coordinates

matrix with its transpose.

Each row of the resulting matrix contains predicted semantic similarities between an item

and all other items. We then compared these predicted similarities to a target similarity matrix

constructed directly from the three components of the original matrix that account for 90% of its

variance. That is, for each item in the dataset, we computed the correlation between the predicted

and true similarities to (a) all other items, (b) other items in the same domain, and (c) other items

in the contrasting domain. For each metric, we then averaged the correlations across (1) all items,

(2) just the animate items or (3) just the inanimate items. These conditions thus allowed us to

assess how well the decoders model semantic similarities both within and across each domain.

The full procedure was carried out independently for each participant at each time-window.

Correlation coefficients in each condition were then averaged across participants at each time-

window.

The results are shown in **Figure 5**. Filled circles indicate where predicted/true

correlations are reliably non-zero relative to a permutation-based null distribution with FDR of p

Figure 5 Correlation between predicted semantic similarities and the best-possible similarities reconstructed from the first three singular vectors/values of the true matrix. Error bars reflect standard error of the mean over participants. Considering all pairwise similarities (left panel green dots), predictions from RSL show much stronger correlations with the true structure than observed in a previous study using searchlight RSA (left panel gray dots; see Y. Chen et al. (2016)). Moreover, where the prior study found no evidence for within-domain semantic structure in these data, decoding models fit with RSL reliably predict semantic similarities both within (orange dots) and between (blue dots) conceptual domains, for both animate (middle panel) and inanimate (right panel) stimuli, from about 100 – 200ms post-stimulus onward.

< 0.05 (Stelzer et al., 2013). Reliable correlations were observed from 100 – 150ms post-

stimulus onward, whether computed across all items, within domain only, or between-domain

only, and considering the full complement of items (left panel), animate items only (middle), or

inanimates only (right). For comparison to RSA, **Figure 5** (left) also shows the mean correlation

(across participants and using the full target matrix) between RSM and NSM at each window

reported in Chen et al.'s (2016) analyses of the same data. While reliably positive correlations

were observed from 200ms onward, the correlation coefficient was about 1/10th the magnitude

observed with RSL (compare with green dots in same panel).

General Discussion

We introduced this paper with a puzzle: neuropsychology, clinical neurophysiology,

TMS, and computational modelling all suggest that the vATLs encode graded and

multidimensional conceptual similarity structure, but direct tests of this hypothesis using

multivariate functional brain imaging have yielded inconclusive and widely heterogeneous

results. Although RSA appears to provide an insightful test of this hypothesis, in simulation we

showed that counter-intuitive limitations of RSA obscure inferences about neurocognitive

representation. When used to decode real semantic structure as measured by feature norms, RSA

can produce positive results even if the underlying neural code is discrete and one-dimensional,

or null results even if the neural code does capture latent structure in the target matrix beyond the

first component. Because RSA relies on an inherently one-dimensional measure of association

(i.e., correlation), it cannot reveal whether neural signals encode multi-dimensional structure.

Because the technique does not fit any parameters to data, it requires the researcher to select

features a priori when constructing the NSM (for instance, via ROI or searchlight analyses; see

Frisby et al., 2023), and cannot learn to ignore irrelevant features amongst those selected. The

simulations suggest that these characteristics of RSA may have contributed to the puzzling state

of the literature—for instance, by yielding results suggesting that vATL only coarsely

discriminates living from nonliving things (Clark & Tyler, 2014; Chen et al., 2015).

RSL addresses these limitations by using regression to predict coordinates of stimuli

along the latent dimensions of the RSM. In simulation, we showed how this approach can

uncover multi-dimensional representational structure (by showing reliable conjoint decoding of

two or more orthogonal dimensions of a target matrix) as well as graded structure (by showing

reliable decoding both within and between semantic domains). The approach can also "select

out" signal-carrying features from amongst those included as predictors in the model, and so can

be applied to all potentially signal-carrying neural features at once, without requiring the theorist

to pre-select an ROI or to look only within small, independent searchlights (see Cox & Rogers,

2021; Frisby et al., 2023).

Applying the approach to large neural datasets requires model regularization. We

illustrated how hypothesized patterns of structured sparsity in the neural signal can constrain

model fit via grOWL regularization and applied this approach to discover semantic structure in

an ECoG dataset where prior work using RSA found only a binary animacy code. In contrast,

RSL with grOWL regularization uncovered a graded and multidimensional semantic space

capturing similarities within and between animate and inanimate domains—consistent with

conclusions drawn about the nature of semantic representations in the ATL hub from other

cognitive and clinical neuroscience sources.

Relevance to category-specific theories of ATL function.

The current results challenge an alternative proposal about the role of ATL in semantic

cognition, namely that they support knowledge of some conceptual categories and not others

(Mahon & Caramazza, 2011; Malone et al., 2016; Simmons et al., 2009). Such a view is

consistent with prior imaging work (e.g., Anzellotti et al., 2011) including the multivariate

decoding studies cited earlier (Y. Chen et al., 2016; Clarke & Tyler, 2014), suggesting that ATL

activations differentiate animates from inanimates but do not otherwise encode or differentiate

finer categories. This alternative perspective has been difficult to reconcile with

neuropsychological evidence showing that anterior temporal atrophy and hypometabolism in

semantic dementia degrades knowledge of animates and inanimates equally (Lambon Ralph et

al., 2007; Noppeney et al., 2007), and with TMS and direct grid stimulation evidence showing

that stimulation of both left and right ATL reliably slows semantic processing for both animates

and artefacts (Pobric et al., 2010; Shimotake et al., 2015). It also struggles to explain the

sensitivity of ATL-related semantic impairment to continuous and graded semantic structure of

test stimuli for both animates and inanimates (Patterson et al., 2006; Rogers et al., 2006). The

current results suggest that prior work may have failed to discover graded cross-domain semantic

structure in ATL responses, not because such structure is absent from the measured responses,

but because limitations in both fMRI and analytic techniques make such structure difficult to

detect.

It is worth noting that intra-domain similarities were more robustly decoded for animate

compared to inanimate items. Considering each dimension separately in the opening window

analysis, within-inanimate decoding was only reliable for the first latent dimension. In the

moving window analysis, where models were trained on 100ms increments of data without the

full history of activation from stimulus onset, within-inanimate decoding was reliable for

components 1 and 3, but transiently. These are the components that best differentiate inanimates

in the target matrix (see Figure 1). When predicting pairwise distances within moving windows,

correlations with true similarities were reliable but smallest for within-inanimate structure (i.e.,

the "other domain" correlations in the middle panel of **Figure 5**, and "same domain" correlations

in the rightmost panel).

We attribute this general pattern to differences, not in the neural code itself, but in the

target similarity structure of animate and inanimate concepts. Semantic subcategories of

inanimate objects are only weakly differentiated, not just in the current dataset, but in norming

studies more generally and in other approaches to characterizing semantic structure (e.g., Devlin

et al., 1998; Garrard et al., 2001; McRae et al., 1997; Tyler et al., 2000). Indeed, this difference

in statistical structure is precisely what leads, under some theories, to apparent category-specific

patterns of semantic impairment (Devlin et al., 2002; Lambon Ralph et al., 2007) and functional

activation (Rogers et al., 2006). The differences can be seen in **Figure 1**, where animate items

fall into somewhat well-differentiated subcategories in components 1 and 2 while inanimates are

uniformly distributed with poorly differentiated subclusters even along component 3.

Accordingly, pairwise similarities reconstructed from the first three singular vectors of the full

semantic matrix are more accurate for animate than inanimate items (see Appendix D). Thus, the

structure of the semantic matrix itself *requires* that decoding be worse within inanimates than

within animates, precisely because inanimates are less well-structured. Yet despite this intrinsic

disadvantage, within-inanimate similarities were still reliably decoded along multiple

components of the embedding and in the reconstructed similarity matrix, illustrating that neural

signal in vATL does express intra-domain semantic structure even for inanimate stimuli.

In summary, the results suggest the vATLs encode a multidimensional representation

space that captures the conceptual similarities existing amongst a variety of different concepts

including both animate and inanimate items (Lambon Ralph et al., 2007; Patterson et al., 2007;

Rogers & McClelland, 2004). Better decoding within animates may reflect the fact that animate

subcategories are better-differentiated, so that intra-domain similarities are better-approximated

by a low-rank decomposition.

We also note that the current results pertain only to the nature of the semantic

information encoded within the span of vATL where electrodes were situated in our patient

sample. They do not bear on claims of possible category-specific representation in other parts of

cortex—for instance, that left infero-parietal cortex and posterior medial temporal gyrus play a

special role in knowledge about tools (Q. Chen et al., 2016; Garcea et al., 2018; Ishibashi et al.,

2016; Kalénine & Buxbaum, 2016) or that earlier visual areas are dedicated to representing

different object categories (Cichy et al., 2014; Connolly et al., 2012; Downing et al., 2001;

Kanwisher et al., 1997; Kriegeskorte, Mur, Ruff, et al., 2008; Mahon et al., 2009; Sha et al.,

2015). Indeed, prior work from (Chen et al., 2017) showed how domain-general semantic

representations can arise in vATL even as graded category-specificity emerges in other parts of

the cortical semantic network, based on empirically-measured patterns of white-matter

connectivity across core areas. Evaluating claims of category-specificity in future work may

benefit from adopting the RSL approach developed here.

Alternative approaches to RSL.

We implemented RSL using multivariate grOWL-regularized regression because the

regularizer captures key information about the hypothesized nature of neurosemantic

representations. That is, the decoding method is directly tied to explicit assumptions about the

neural code we aim to discover, as recommended by Frisby et al. (2023). Still, there exist other

techniques for modeling the relationship between neural and target similarity structures that

embody other representational assumptions and are worth exploring (see Oswal et al., 2016 for

comparisons to some other related methods). Aside from the grOWL approach and the results we

have reported, the current paper makes two broader contributions. First, claims of graded multi-

dimensional representation in neural activity should be supported by evidence that neural signals

encode structure along multiple orthogonal components of a matrix, at multiple granularities.

Second, results can vary significantly depending upon the decoding technique applied, so the

method chosen should be justified with reference to explicit hypotheses about the nature of the

underlying code.

Implications for the broader literature.

The characteristics of RSA we have identified carry additional implications for interpretation of the broader literature. A recent review (Frisby et al., 2023) identified 34 studies that have applied RSA to the discovery of semantic representations in the brain, with positive results observed across multiple cortical regions including posterior temporal cortex (Connolly et al., 2012), angular gyrus (Fairhall & Caramazza, 2013; Fernandino et al., 2022), left perisylvian cortex (Devereux et al., 2013), and prefrontal cortex (Carota et al., 2017). Simulation 1 suggests, however, that RSA will yield a positive result for any property correlated with the animate/inanimate distinction, including even discrete binary properties. Many features are confounded with animacy: inanimate items tend to be more familiar, less visually complex, more associated with action plans, less associated with motion, more likely to have lines and corners, less predictable from color or texture, etc. (see Chen & Rogers, 2014 for a review). Most RSA papers do not report the magnitude of correlation between RSM and NSM where results are significant, instead focusing on whether the estimated correlation coefficient is reliably non-zero across participants. As shown by the prior RSA analysis of the same ECoG data explored here (Y. Chen et al., 2016; gray line in Figure 5), this can happen even when mean correlations are very small. Moreover, several studies use target RSMs with only a small number of rows/columns—sometimes as few as five (Connolly et al., 2012; Fairhall & Caramazza, 2013), meaning that correlations are computed across just 10 cells of the matrix (i.e., the lower triangle of a 5x5 RSM). Such small numbers increase the likelihood that a small-but-non-zero correlation is driven by some arbitrary property of the chosen stimuli or categories. Together these observations raise the possibility that the literature contains misleading positive results—brain areas whose responses encode unidimensional characteristics weakly confounded with animacy,

732   rather than multi-dimensional semantic structure. Testing this possibility for various brain areas

733   hypothesized to encode semantic structure will require analyses like those we have developed

734   here.

735   **Conclusion**

736   In cognitive science, semantic representations are often construed as vector spaces that

encoded graded, multidimensional similarity structure amongst the concepts experienced in our

verbal and nonverbal world. Through application of a new technique for mapping

representational similarity in neural activity, we have shown that neural signals in vATL encode

such a space. In so doing, we have identified some limitations of representational similarity

analysis, a widespread technique commonly thought to reveal graded and multidimensional

representational structure. The work resolves an important discrepancy between behavioral and

neuroimaging results in prior work and suggests a new approach to discovering representational

structure in neural data more generally.

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Data and materials availability: RSL models were fit using the WISC MVPA toolbox

(https://github.com/crcox/WISC_MVPA). Analysis of RSL models was conducted using custom

MATLAB code (https://github.com/crcox/RSL_correlation_analysis), and the data and script

necessary to replicate them is available via the Open Science Framework (https://osf.io/axseq/).

R scripts for generating figures based on the correlation analyses are on GitHub

(https://github.com/crcox/ecog-rsl-figures).

Appendices:

References

Abel, T. J., Rhone, A. E., Nourski, K. V., Kawasaki, H., Oya, H., Griffiths, T. D., Howard, M.
     A., 3rd, & Tranel, D. (2015). Direct physiologic evidence of a heteromodal convergence
     region for proper naming in human left anterior temporal lobe. *Journal of Neuroscience*,
     35(4), 1513-1520. https://doi.org/10.1523/JNEUROSCI.3387-14.2015

Acosta-Cabronero, J., Patterson, K., Fryer, T. D., Hodges, J. R., Pengas, G., Williams, G. B., &
     Nestor, P. J. (2011). Atrophy, hypometabolism and white matter abnormalities in
     semantic dementia tell a coherent story. *Brain*, *134*(7), 2025-2035.
     https://doi.org/10.1093/brain/awr119

Anzellotti, S., Mahon, B. Z., Schwarzbach, J., & Caramazza, A. (2011). Differential activity for
     animals and manipulable objects in the anterior temporal lobes. *J Cogn Neurosci*, *23*(8),
     2059-2067. https://doi.org/10.1162/jocn.2010.21567

Binder, J. R., & Desai, R. H. (2011). The neurobiology of semantic memory. *Trends in Cognitive
     Sciences*, *15*(11), 527-536. https://doi.org/10.1016/j.tics.2011.10.001

Binder, J. R., Desai, R. H., Graves, W. W., & Conant, L. L. (2009). Where is the semantic
     system? A critical review and meta-analysis of 120 functional neuroimaging studies.
     Cerebral Cortex, *19*(12), 2767-2796. https://doi.org/10.1093/cercor/bhp055

Binney, R. J., Embleton, K. V., Jefferies, E., Parker, G. J. M., & Lambon Ralph, M. A. (2010).
     The ventral and inferolateral aspects of the anterior temporal lobe are crucial in semantic
     memory: evidence from a novel direct comparison of distortion-corrected fMRI, rTMS,
     and semantic dementia. *Cerebral Cortex*, *20*(11), 2728-2738.
     https://doi.org/10.1093/cercor/bhq019

798   Binney, R. J., & Lambon Ralph, M. A. (2015). Using a combination of fMRI and anterior

799   temporal lobe rTMS to measure intrinsic and induced activation changes across the

800   semantic cognition network. *Neuropsychologia*, *76*, 170-181.

801   https://doi.org/10.1016/j.neuropsychologia.2014.11.009

802   Bruffaerts, R., Dupont, P., Peeters, R., De Deyne, S., Storms, G., & Vandenberghe, R. (2013).

803   Similarity of fMRI activity patterns in left perirhinal cortex reflects semantic similarity

804   between words. *Journal of Neuroscience*, *33*(47), 18597-18607.

805   https://doi.org/10.1523/JNEUROSCI.1548-13.2013

806   Carota, F., Kriegeskorte, N., Nili, H., & Pulvermuller, F. (2017). Representational Similarity

807   Mapping of Distributional Semantics in Left Inferior Frontal, Middle Temporal, and

808   Motor Cortex. *Cerebral Cortex*, *27*(1), 294-309. https://doi.org/10.1093/cercor/bhw379

809   Carota, F., Nili, H., Pulvermüller, F., & Kriegeskorte, N. (2021). Distinct fronto-temporal

810   substrates of distributional and taxonomic similarity among words: evidence from RSA

811   of BOLD signals. *NeuroImage*, *224*, 117408.

812   https://doi.org/10.1016/j.neuroimage.2020.117408

813   Chao, L. L., Haxby, J. V., & Martin, A. (1999). Attribute-based neural substrates in temporal

814   cortex for perceiving and knowing about objects. *Nature Neuroscience*, *2*(10), 913-919.

815   https://doi.org/10.1038/13217

816   Chen, L., Lambon Ralph, M. A., & Rogers, T. T. (2017). A unified model of human semantic

817   knowledge and its disorders. *Nature Human Behaviour*, *1*(3), 1-10.

818   https://doi.org/10.1038/s41562-016-0039

Chen, L., & Rogers, T. T. (2014). Revisiting domain-general accounts of category specificity in

mind and brain. *WIREs Cognitive Science*, *5*(3), 327-344.

https://doi.org/10.1002/wcs.1283

Chen, Q., Garcea, F. E., & Mahon, B. Z. (2016). The Representation of Object-Directed Action

and Function Knowledge in the Human Brain. *Cereb Cortex*, *26*(4), 1609-1618.

https://doi.org/10.1093/cercor/bhu328

Chen, Y., Shimotake, A., Matsumoto, R., Kunieda, T., Kikuchi, T., Miyamoto, S., Fukuyama,

H., Takahashi, R., Ikeda, A., & Lambon Ralph, M. A. (2016). The 'when' and 'where' of

semantic coding in the anterior temporal lobe: Temporal representational similarity

analysis of electrocorticogram data. *Cortex*, *79*, 1-13.

https://doi.org/10.1016/j.cortex.2016.02.015

Cichy, R. M., Pantazis, D., & Oliva, A. (2014). Resolving human object recognition in space and

time. *Nature Neuroscience*, *17*(3), 455. https://doi.org/10.1038/nn.3635

Clarke, A., & Tyler, L. K. (2014). Object-specific semantic coding in human perirhinal cortex.

Journal of Neuroscience, *34*(14), 4766-4775. https://doi.org/10.1523/JNEUROSCI.2828-

13.2014

Connolly, A. C., Guntupalli, J. S., Gors, J., Hanke, M., Halchenko, Y. O., Wu, Y.-C., Abdi, H.,

& Haxby, J. V. (2012). The representation of biological classes in the human brain.

Journal of Neuroscience, *32*(8), 2608-2618. https://doi.org/10.1523/JNEUROSCI.5547-

11.2012

Cox, C. R. (2021). *Whole-brain Imaging with Sparse Correlations*. In Github.

Cox, C. R., & Rogers, T. T. (2021). Finding Distributed Needles in Neural Haystacks. *Journal of

Neuroscience*, *41*(5), 1019-1032. https://doi.org/10.1523/jneurosci.0904-20.2020

Devereux, B. J., Clarke, A., Marouchos, A., & Tyler, L. K. (2013). Representational Similarity

Analysis Reveals Commonalities and Differences in the Semantic Processing of Words

and Objects. *Journal of Neuroscience*, *33*(48), 18906-18916.

https://doi.org/10.1523/jneurosci.3809-13.2013

Devereux, B. J., Clarke, A., & Tyler, L. K. (2018). Integrated deep visual and semantic attractor

neural networks predict fMRI pattern-information along the ventral object processing

pathway. *Scientific reports*, *8*(1), 10636. https://doi.org/10.1038/s41598-018-28865-1

Devlin, J. T., Gonnerman, L. M., Andersen, E. S., & Seidenberg, M. S. (1998). Category-

Specific Semantic Deficits in Focal and Widespread Brain Damage: A Computational

Account [Article]. *Journal of Cognitive Neuroscience*, *10*(1), 77-94.

https://doi.org/10.1162/089892998563798

Devlin, J. T., Russell, R. P., Davis, M. H., Price, C. J., Moss, H. E., Fadili, M. J., & Tyler, L. K.

(2002). Is there an anatomical basis for category-specificity? Semantic memory studies in

PET and fMRI. *Neuropsychologia*, *40*(1), 54-75. https://doi.org/10.1016/S0028-

3932(01)00066-5

Dilkina, K., & Lambon Ralph, M. A. (2013). Conceptual structure within and between

modalities. *Frontiers in Human Neuroscience*, *6*, 333.

https://doi.org/10.3389/fnhum.2012.00333

Downing, P. E., Jiang, Y., Shuman, M., & Kanwisher, N. (2001). A cortical area selective for

visual processing of the human body. *Science*, *293*(5539), 2470-2473.

https://doi.org/10.1126/science.1063414

Drane, D. L., Ojemann, G. A., Aylward, E., Ojemann, J. G., Johnson, L. C., Silbergeld, D. L.,

Miller, J. W., & Tranel, D. (2008). Category-specific naming and recognition deficits in

temporal lobe epilepsy surgical patients. *Neuropsychologia*, *46*(5), 1242-1255.

https://doi.org/https://doi.org/10.1016/j.neuropsychologia.2007.11.034

Edgington, E., & Onghena, P. (2007). *Randomization Tests* (4th ed.) [Book]. Chapman and

Hall/CRC.

Fairhall, S. L., & Caramazza, A. (2013). Brain regions that represent amodal conceptual

knowledge. *Journal of Neuroscience*, *33*(25), 10552-10558.

https://doi.org/10.1523/JNEUROSCI.0051-13.2013

Fernandino, L., Tong, J.-Q., Conant, L. L., Humphries, C. J., & Binder, J. R. (2022). Decoding

the information structure underlying the neural representation of concepts. *Proceedings*

of the National Academy of Sciences, *119*(6), e2108091119.

https://doi.org/doi:10.1073/pnas.2108091119

Figueiredo, M., & Nowak, R. (2016). Ordered weighted l1 regularized regression with strongly

correlated covariates: Theoretical aspects. Artificial Intelligence and Statistics,

Frisby, S. L., Halai, A. D., Cox, C. R., Lambon Ralph, M. A., & Rogers, T. T. (2023). Decoding

semantic representations in mind and brain. *Trends Cogn Sci*, *27*(3), 258-281.

https://doi.org/10.1016/j.tics.2022.12.006

Gainotti, G. (2018). Why do herpes simplex encephalitis and semantic dementia show a different

pattern of semantic impairment in spite of their main common involvement within the

anterior temporal lobes? *Rev Neurosci*, *29*(3), 303-320. https://doi.org/10.1515/revneuro-

2017-0034

Garcea, F. E., Chen, Q., Vargas, R., Narayan, D. A., & Mahon, B. Z. (2018). Task- and domain-

specific modulation of functional connectivity in the ventral and dorsal object-processing

887   pathways. *Brain Struct Funct*, *223*(6), 2589-2607. https://doi.org/10.1007/s00429-018-

888   1641-1

889   Garrard, P., Lambon Ralph, M. A., Hodges, J. R., & Patterson, K. (2001). Prototypicality,

890   distinctiveness, and intercorrelation: Analyses of the semantic attributes of living and

891   nonliving concepts [Article]. *Cognitive neuropsychology*, *18*(2), 125-174.

892   https://doi.org/10.1080/02643290125857

893   Halai, A. D., Parkes, L. M., & Welbourne, S. R. (2015). Dual-echo fMRI can detect activations

894   in inferior temporal lobe during intelligible speech comprehension. *NeuroImage*, *122*,

895   214-221. https://doi.org/10.1016/j.neuroimage.2015.05.067

896   Halai, A. D., Welbourne, S. R., Embleton, K., & Parkes, L. M. (2014). A comparison of dual

897   gradient-echo and spin-echo fMRI of the inferior temporal lobe. *Human brain mapping*,

898   *35*(8), 4118-4128. https://doi.org/10.1002/hbm.22463

899   Haxby, J. V., Gobbini, M. I., Furey, M. L., Ishai, A., Schouten, J. L., & Pietrini, P. (2001).

900   Distributed and overlapping representations of faces and objects in ventral temporal

901   cortex. *Science*, *293*(5539), 2425-2430. https://doi.org/10.1126/science.1063736

902   Hebart, M. N., Zheng, C. Y., Pereira, F., & Baker, C. I. (2020). Revealing the multidimensional

903   mental representations of natural objects underlying human similarity judgements. *Nature*

904   *Human Behaviour*, *4*(11), 1173-1185. https://doi.org/10.1038/s41562-020-00951-3

905   Hodges, J. R., & Patterson, K. (2007). Semantic dementia: a unique clinicopathological

906   syndrome [Review Article]. *Lancet Neurology*, *6*(11), 1004-1014.

907   https://doi.org/10.1016/S1474-4422(07)70266-1

908   Huth, A. G., de Heer, W. A., Griffiths, T. L., Theunissen, F. E., & Gallant, J. L. (2016). Natural

909   speech reveals the semantic maps that tile human cerebral cortex. *Nature*, *532*(7600),

910   453-458. https://doi.org/10.1038/nature17637

911   Ishibashi, R., Pobric, G., Saito, S., & Lambon Ralph, M. A. (2016). The neural network for tool-

912   related cognition: An activation likelihood estimation meta-analysis of 70 neuroimaging

913   contrasts. *Cogn Neuropsychol*, *33*(3-4), 241-256.

914   https://doi.org/10.1080/02643294.2016.1188798

915   Jackson, R. L., Rogers, T. T., & Lambon Ralph, M. A. (2021). Reverse-engineering the cortical

916   architecture for controlled semantic cognition. *Nature Human Behaviour*.

917   https://doi.org/10.1038/s41562-020-01034-z

918   Jefferies, E. (2013). The neural basis of semantic cognition: Converging evidence from

919   neuropsychology, neuroimaging and TMS. *Cortex*, *49*(3), 611-625.

920   https://doi.org/10.1016/j.cortex.2012.10.008

921   Kalénine, S., & Buxbaum, L. J. (2016). Thematic knowledge, artifact concepts, and the left

922   posterior temporal lobe: Where action and object semantics converge. *Cortex*, *82*, 164-

923   178. https://doi.org/10.1016/j.cortex.2016.06.008

924   Kanwisher, N., McDermott, J., & Chun, M. M. (1997). The fusiform face area: A module in

925   human extrastriate cortex specialized for face perception. *Journal of Neuroscience*,

926   *17*(11), 4302-4311. https://doi.org/10.1523/JNEUROSCI.17-11-04302.1997

927   Kriegeskorte, N., Mur, M., & Bandettini, P. A. (2008). Representational similarity analysis -

928   connecting the branches of systems neuroscience. *Frontiers in Systems Neuroscience*, *2*,

929   4. https://doi.org/10.3389/neuro.06.004.2008

Kriegeskorte, N., Mur, M., Ruff, D. A., Kiani, R., Bodurka, J., Esteky, H., Tanaka, K., &

Bandettini, P. A. (2008). Matching categorical object representations in inferior temporal

cortex of man and monkey. *Neuron*, *60*(6), 1126-1141.

https://doi.org/10.1016/j.neuron.2008.10.043

Lambon Ralph, M. A. (2014). Neurocognitive insights on conceptual knowledge and its

breakdown. *Philosophical Transactions of the Royal Society B: Biological Sciences*,

369(1634), 20120392. https://doi.org/10.1098/rstb.2012.0392

Lambon Ralph, M. A., Jefferies, E., Patterson, K., & Rogers, T. T. (2017). The neural and

computational bases of semantic cognition. *Nature Reviews Neuroscience*, *18*(1), 42.

https://doi.org/10.1038/nrn.2016.150

Lambon Ralph, M. A., Lowe, C., & Rogers, T. T. (2007). Neural basis of category-specific

semantic deficits for living things: evidence from semantic dementia, HSVE and a neural

network model. *Brain*, *130*, 1127-1137. https://doi.org/10.1093/brain/awm025

Lambon Ralph, M. A., Pobric, G., & Jefferies, E. (2009). Conceptual knowledge is underpinned

by the temporal pole bilaterally: convergent evidence from rTMS. *Cereb Cortex*, *19*(4),

832-838. https://doi.org/10.1093/cercor/bhn131

Li, L., Jamieson, K., DeSalvo, G., Rostamizadeh, A., & Talwalkar, A. (2018). Hyperband: A

Novel Bandit-Based Approach to Hyperparameter Optimization [Article]. *Journal of

Machine Learning Research*, *18*(154-234), 1-52.

Mahon, B. Z., Anzellotti, S., Schwarzbach, J., Zampini, M., & Caramazza, A. (2009). Category-

specific organization in the human brain does not require visual experience. *Neuron*,

63(3), 397-405. https://doi.org/10.1016/j.neuron.2009.07.012

Mahon, B. Z., & Caramazza, A. (2011). What drives the organization of object knowledge in the

953   brain? *Trends in Cognitive Sciences*, *15*(3), 97-103.

954   https://doi.org/10.1016/j.tics.2011.01.004

955   Malone, P. S., Glezer, L. S., Kim, J., Jiang, X., & Riesenhuber, M. (2016). Multivariate Pattern

956   Analysis Reveals Category-Related Organization of Semantic Representations in

957   Anterior Temporal Cortex. *J Neurosci*, *36*(39), 10089-10096.

958   https://doi.org/10.1523/JNEUROSCI.1599-16.2016

959   Martin, A. (2007). The representation of object concepts in the brain. *Annual review of*

960   *psychology*, *58*, 25-45. https://doi.org/10.1146/annurev.psych.57.102904.190143

961   Martin, A. (2016). GRAPES--Grounding representations in action, perception, and emotion

962   systems: How object properties and categories are represented in the brain. *Psychonomic*

963   *Bulletin & Review*, *23*, 979 -- 990. https://doi.org/10.3758/s13423-015-0842-3

964   Martin, C. B., Douglas, D., Newsome, R. N., Man, L. L. Y., & Barense, M. D. (2018).

965   Integrative and distinctive coding of visual and conceptual object features in the ventral

966   visual stream. *Elife*, *7*, e31873. https://doi.org/10.7554/eLife.31873

967   MathWorks. (2018). *Matlab*. In *MATLAB* (Version 9.5 (R2018b)) The MathWorks.

968   McRae, K., Cree, G. S., Seidenberg, M. S., & McNorgan, C. (2005). Semantic feature production

969   norms for a large set of living and nonliving things. *Behavior research methods*, *37*(4),

970   547-559. https://doi.org/10.3758/BF03192726

971   McRae, K., de Sa, V. R., & Seidenberg, M. S. (1997). On the nature and scope of featural

972   representations of word meaning. *Journal of Experimental Psychology: General*, *126*(2),

973   99-130. https://doi.org/10.1037/0096-3445.126.2.99

Noppeney, U., Patterson, K., Tyler, L. K., Moss, H., Stamatakis, E. A., Bright, P., Mummery, C.,

& Price, C. J. (2007). Temporal lobe lesions and semantic impairment: a comparison of

herpes simplex virus encephalitis and semantic dementia. *Brain*, *130*(Pt 4), 1138-1147.

https://doi.org/10.1093/brain/awl344

Oswal, U., Cox, C. R., Lambon Ralph, M. A., Rogers, T. T., & Nowak, R. D. (2016).

Representational similarity learning with application to brain networks. ICML'16

Proceedings of the 33rd International Conference on International Conference on

Machine Learning, New York, USA.

Oswal, U., & Nowak, R. (2018, 2-5 Oct. 2018). Scalable Sparse Subspace Clustering via

Ordered Weighted l1 Regression. 2018 56th Annual Allerton Conference on

Communication, Control, and Computing (Allerton),

Patterson, K., Nestor, P. J., & Rogers, T. T. (2007). Where do you know what you know? The

representation of semantic knowledge in the human brain. *Nature Reviews Neuroscience*,

8(12), 976-987. https://doi.org/10.1038/nrn2277

Patterson, K., Ralph, M. A. L., Jefferies, E., Woollams, A., Jones, R., Hodges, J. R., & Rogers,

T. T. (2006). "Presemantic" Cognition in Semantic Dementia: Six Deficits in Search of

an Explanation. *Journal of Cognitive Neuroscience*, *18*(2), 169-183.

https://doi.org/10.1162/jocn.2006.18.2.169

Peelen, M. V., & Caramazza, A. (2012). Conceptual object representations in human anterior

temporal cortex. *Journal of Neuroscience*, *32*(45), 15728-15736.

https://doi.org/10.1523/JNEUROSCI.1953-12.2012

Pereira, F., Gershman, S., Ritter, S., & Botvinick, M. (2016). A comparative evaluation of off-

the-shelf distributed semantic representations for modelling behavioural data. *Cognitive*

neuropsychology, *33*(3-4), 175-190. https://doi.org/10.1080/02643294.2016.1176907

Phipson, B., & Smyth, G. K. (2010). Permutation P-values Should Never Be Zero: Calculating

Exact P-values When Permutations Are Randomly Drawn. *Statistical Applications in*

Genetics and Molecular Biology, *9*(1). https://doi.org/10.2202/1544-6115.1585

Pobric, G., Jefferies, E., & Lambon Ralph, M. A. (2007). Anterior temporal lobes mediate

semantic representation: mimicking semantic dementia by using rTMS in normal

participants. *Proceedings of the National Academy of Sciences*, *104*(50), 20137-20141.

https://doi.org/10.1073/pnas.0707383104

Pobric, G., Jefferies, E., & Lambon Ralph, M. A. (2010). Category-specific versus category-

general semantic impairment induced by transcranial magnetic stimulation. *Current*

Biology, *20*(10), 964-968. https://doi.org/10.1016/j.cub.2010.03.070

Rogers, T. T., Cox, C. R., Lu, Q., Shimotake, A., Kikuchi, T., Kunieda, T., Miyamoto, S.,

Takahashi, R., Ikeda, A., Matsumoto, R., & Lambon Ralph, M. A. (2021). Evidence for a

deep, distributed and dynamic code for animacy in human ventral anterior temporal

cortex. *Elife*, *10*, e66276. https://doi.org/10.7554/eLife.66276

Rogers, T. T., Hocking, J., Noppeney, U., Mechelli, A., Gorno-Tempini, M. L., Patterson, K., &

Price, C. J. (2006). Anterior temporal cortex and semantic memory: reconciling findings

from neuropsychology and functional imaging. *Cognitive, Affective, & Behavioral*

Neuroscience, *6*(3), 201-213. https://doi.org/10.3758/CABN.6.3.201

Rogers, T. T., Lambon Ralph, M. A., Garrard, P., Bozeat, S., McClelland, J. L., Hodges, J. R., &

Patterson, K. (2004). Structure and Deterioration of Semantic Memory: A

Neuropsychological and Computational Investigation. *Psychological Review*, *111*(1),

205-235. https://doi.org/10.1037/0033-295X.111.1.205

Rogers, T. T., & McClelland, J. L. (2004). *Semantic cognition: A parallel distributed processing*

approach. MIT press.

Rogers, T. T., & McClelland, J. L. (2014). Parallel Distributed Processing at 25: further

explorations in the microstructure of cognition. *Cognitive Science*, *38*(6), 1024-1077.

https://doi.org/10.1111/cogs.12148

Schapiro, A. C., McClelland, J. L., Welbourne, S. R., Rogers, T. T., & Lambon Ralph, M. A.

(2013). Why bilateral damage is worse than unilateral damage to the brain. *J Cogn*

Neurosci, *25*(12), 2107-2123. https://doi.org/10.1162/jocn_a_00441

Sha, L., Haxby, J. V., Abdi, H., Guntupalli, J. S., Oosterhof, N. N., Halchenko, Y. O., &

Connolly, A. C. (2015). The animacy continuum in the human ventral vision pathway.

Journal of Cognitive Neuroscience, *27*(4), 665-678.

https://doi.org/10.1162/jocn_a_00733

Shimotake, A., Matsumoto, R., Ueno, T., Kunieda, T., Saito, S., Hoffman, P., Kikuchi, T.,

Fukuyama, H., Miyamoto, S., Takahashi, R., Ikeda, A., & Lambon Ralph, M. A. (2015).

Direct Exploration of the Role of the Ventral Anterior Temporal Lobe in Semantic

Memory: Cortical Stimulation and Local Field Potential Evidence From Subdural Grid

Electrodes. *Cerebral Cortex*, *25*(10), 3802-3817. https://doi.org/10.1093/cercor/bhu262

Simmons, W. K., Reddish, M., Bellgowan, P. S. F., & Martin, A. (2009). The Selectivity and

Functional Connectivity of the Anterior Temporal Lobes. *Cerebral Cortex*, *20*(4), 813-

825. https://doi.org/10.1093/cercor/bhp149

Snowden, J. S., Goulding, P. J., & Neary, D. (1989). Semantic dementia: A form of

circumscribed cerebral atrophy. *Behavioural Neurology*.

https://doi.org/10.1155/1989/124043

Stelzer, J., Chen, Y., & Turner, R. (2013). Statistical inference and multiple testing correction in

classification-based multi-voxel pattern analysis (MVPA): random permutations and

cluster size control. *NeuroImage*, *65*, 69-82.

https://doi.org/10.1016/j.neuroimage.2012.09.063

Tyler, L. K., Moss, H. E., Durrant-Peatfield, M. R., & Levy, J. P. (2000). Conceptual Structure

and the Structure of Concepts: A Distributed Account of Category-Specific Deficits.

Brain and Language, *75*(2), 195-231. https://doi.org/10.1006/brln.2000.2353

Yuan, M., & Lin, Y. (2006). Model selection and estimation in regression with grouped

variables. *Journal of the Royal Statistical Society: Series B (Statistical Methodology)*,

68(1), 49-67. https://doi.org/10.1111/j.1467-9868.2005.00532.x

Zhou, Y., Vales, M. I., Wang, A., & Zhang, Z. (2017). Systematic bias of correlation coefficient

may explain negative accuracy of genomic prediction. *Briefings in Bioinformatics*, *18*(6),

1093-1093. https://doi.org/10.1093/bib/bbx133

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1058 **Appendix A: Categorized experimental stimuli**

1059 Table S1. Categorized experimental stimuli

Domain	Category	Words
Animate	*Bird*	duck, eagle, ostrich, owl, peacock, penguin, rooster, swan
	Bug	ant, bee, butterfly, caterpillar, fly, ladybird, snail, spider
	Land	bat, bear, camel, cat, cow, deer, dog, dragon, elephant, fox, frog, giraffe, goat, gorilla, horse, kangaroo, lion, monkey, mouse, pig, rabbit, raccoon, rhinoceros, sheep, snake, squirrel, tiger, tortoise, zebra
	Water	crab, fish, lobster, seahorse, whale
Inanimate	*Clothes*	dress, glove, mitten, skirt
	Music	bell, cymbals, drum, flute, guitar, harp, piano, trumpet, violin, whistle
	Object	anchor, barrel, basket, cake, cannon, chain, church, cigar, clock, crown, fence, gun, hammer, iron, kite, ladder, nut, pram, shell, slide, snowman, suitcase, swing, toaster, vase, web, wheel, windmill, yoyo
	Vehicle	aeroplane, helicopter, motorcycle, ski, sled, tractor, train

1060

1061   **Appendix B: Formal description of the RSL approach.**

Let S be a symmetric $n \times n$ target matrix of approximate rank r describing pairwise

cognitive similarities amongst n items, which is decomposed via singular-value decomposition

(SVD) into an $n \times r$ matrix U of r orthonormal singular vectors and an $r \times r$ diagonal matrix D

containing the corresponding r singular values (**Figure 2A**). The matrix product $U\sqrt{D}$ then

contains root-weighted singular vectors that can be viewed as encoding the coordinates of each

stimulus within an r-dimensional latent semantic space, while the product of this matrix with its

transpose provides a rank r approximation of the original similarity matrix. That is:

1069 $$S_{n \times n} \cong U_{n \times r} D_{r \times r} U^T = U\sqrt{D}\,(U\sqrt{D})^T$$

Let $X_{n \times m}$ be a data matrix recording neural responses to each of n stimuli over m neural

features (e.g., voxels in fMRI, electrode voltages at each timepoint in ECoG, etc.). To assess

whether some weighted combination of these features jointly encode the target similarities, we

seek a *decoding matrix* $\beta_{m \times r}$ such that the matrix product $X\beta$ produces r coordinates for each

item, deviating as little as possible from those in target matrix $U\sqrt{D}$. This search can be

formulated as the convex optimization:

1076 $$argmin_\beta \left\| U\sqrt{D} - X\beta \right\|_F$$

That is, we seek β values that minimize the Froebenius norm (i.e., sum of squared

differences) between the true root-weighted singular vectors $U\sqrt{D}$ and the predicted values $X\beta$.

The optimization essentially computes a simultaneous regression predicting all r coordinates for

each stimulus from weighted combinations of the neural responses they evoke. Each column of

the resulting decoding matrix contains one coefficient for each neural feature and predicts an

item's coordinate along one component of the target matrix $U\sqrt{D}$ (ie, one dimension of the

semantic space).

As noted earlier, there are typically many more neural measurements (predictors) than

stimuli (i.e., target data points)—that is, $m \gg n$. Thus, the optimization just defined is under-

constrained and must be regularized with an additional loss H, itself a function of the coefficient

matrix $\boldsymbol{\beta}$:

$$argmin_\beta \left(\left\| U\sqrt{D} - X\beta \right\|_F + \alpha H(\beta) \right)$$

…which is also convex so that a weighted sum of this function and the original

reconstruction loss together yield a single unique solution that can be discovered via gradient

descent. The constant α is a free weighting parameter governing the importance of the

regularization loss relative to the model error.

For RSL we wish to use a regularization function that promotes solutions respecting the

sparsity, redundancy, and spanning assumptions described earlier. Oswal et al. (2016) formulated

a regularizer that accomplishes these objectives by constraining the structure of the decoding

matrix $\boldsymbol{\beta}$ in a single convex loss called the *group ordered weighted LASSO* or *grOWL*. The

approach generalizes both the group LASSO (Yuan & Lin, 2006) and the ordered-weighted

LASSO (Figueiredo & Nowak, 2016) to favor solutions that are (1) row-sparse (rows of $\boldsymbol{\beta}$ are

either all zero or all non-zero), implementing both the sparsity and spanning constraints, but (2)

with subgroups of selected features sharing similar coefficients if their activations covary

strongly together (implementing the redundancy constraint). The grOWL loss is specified as:

$$H(\beta) = \sum_{i=1}^{m} w_i \left\| \beta_{[i]\cdot} \right\|_2$$

Here m is the number of neural features (rows of $\boldsymbol{\beta}$), $\boldsymbol{\beta}_{[i]\cdot}$ is the row of $\boldsymbol{\beta}$ with the i-th

largest 2-norm (i.e., the ith longest coefficient vector), and w_i is a vector of non-negative, non-

increasing weights (for instance a vector of positive values that decay linearly from an initial

constant). Intuitively the loss works as follows. The first element of the weighting vector w is

stipulated to be as large or larger than all other elements, and this weight is applied to whichever

neural feature has the largest coefficients in the decoding matrix (i.e., the 2-norm or length of the

corresponding row). Thus, the feature with the largest coefficients exerts the largest

regularization cost. The optimization must therefore put the largest weights on the most

informative feature to make it "worth" the high regularization cost. If the most informative

feature is also correlated with many other features, their total cost can be further minimized by

placing similar weights across all such features, since the cost for each such weight declines with

the weight sequence in w. Thus, grOWL spontaneously clusters correlated signal-carrying neural

features and gives these a similar weight, effectively averaging them. Finally, the weighting

vector ensures that coefficients on features that do not reduce error beyond those already selected

will be pressured to zero, ensuring overall sparsity. Formal analysis of the grOWL regularizer

and mathematical proofs of its row-sparse and clustering properties were provided by Oswal et

al. (2016).

1120

1121   **Appendix C: RSL and negative correlations**

1122   The analysis protocol presented in this paper involves generating out-of-sample

predictions with k-fold cross validation and then aggregating those test-set predictions into a

single matrix before correlating with the target embedding all in one go. This is in contrast with a

more conventional protocol in which the performance metric is computed separately within each

fold and then averaged. When the metric is something like mean squared error or classification

accuracy, the two protocols are equivalent. With correlation, however, the two protocols yield

different values.

1129   Pearson's r compares variables with zero mean and unit variance. Consequently, when

correlations between target and predicted embeddings are computed separately by holdout-set,

the scale of the predictions relative to the target is disregarded. By aggregating over test sets and

correlating one time, the standardization is done at the level of the full dataset and not for

individual test sets. We feel this is a better metric of whether our models can embed all items

appropriately within the target similarity space—it matters how items are situated with respect to

one another even if they are in different test sets.

1136   When models are fit with cross validation, the targets (and the data) are standardized with

1137   respect to the values in the training set. Thus, the model predictions, including test set

1138   predictions, are on the scale of the standardized *training set*. This means that, to aggregate over

1139   test sets and correlate with the full set of targets, the mean and variance of the target embeddings

1140   in the *training set* need to be added back into the predictions for the corresponding *test set.*

1141   Applying this adjustment will introduce negative correlations between target and

predicted embeddings for models that have been regularized to have weights that are all zero.

This will happen when relationships between the neural data and the target embedding is weak or

non-existent, because putting a weight on any neural feature increases the model cost function

without reducing the prediction error on the training set. In such cases, the unadjusted model

predictions will all be zero, and the adjusted predictions will be the mean of the training set. If

the mean of the training set is greater than the grand mean of the full set, then the mean of the

test set must be less than the grand mean of the full set. Thus, adjusted and aggregated test set

predictions will be negatively correlated with the full target embedding when the model has all

zero (or trivially small) weights due to the LASSO or grOWL regularization penalty. These

concepts are illustrated in Figure S1 in an imagined case where all-zero models are learned on

each of three cross-validation folds.

1153   What we found in practice is that grOWL is "more aggressive" about assigning zero or

trivially small weights than LASSO in the earliest and smallest time-windows. We consider this

to be desirable behavior because we do not expect much semantic activity in the ATLs at 50ms

post stimulus onset. Figure S2 is analogous to Figure 4 in the main paper, except that the

correlation values are not centered on the mean of their corresponding permutation distribution.

This reveals the negative correlations between grOWL model predictions and the target

embedding for small windows where we do not expect semantic activation to be reliably present,

and general consistency of performance elsewhere. These negative correlations are an expected

artifact of our analysis protocol and do not change the interpretation of our results.

Figure S1 A schematic depiction of the relationship between test sets, training set means, the sample grand mean, and model predictions when the model consists of zero-weights on all neural features. A zero-weight model can occur when model regularization involves the LASSO penalty and the cost of applying a non-zero weight does not outweigh the benefit of reducing prediction error. If the mean of the test set differs from the grand mean, the mean of the test set must also differ from the grand mean. Importantly, if the mean of the test set is less than the grand mean, the mean of the training set must be higher. Unadjusted predictions (i.e., those that ignore the mean of the training set) will be all zero when the model weights are all zero; adjusted predictions are scaled by the training set mean. Leads to systematically negative correlations between true and predicted values for models regularized to have all-zero weights.

Figure S2. Uncentered ECoG decoding results. This figure is completely analogous to Figure 4 in the main paper, except that the raw correlations are presented, without centering on the mean of the permutation distribution. We see that the predictions of models fit with grOWL to small windows, including the least activation since stimulus onset, tend to be negatively correlated with the target values. This is due to the models being assigned very small weights, such that the variance in the predicted values associated with the training set means is large relative to the variance associated with the variability in the neural data. It is possible for negative correlations to be reliably higher than the expected value until the permutation-simulated null, as seen for the animate-subordinate structure along dimension 2 in the 200-ms window.

1162

                    Appendix D: Reconstructing item similarity from SVD coordinates

1164   The main analysis uses the first three root-weighted singular vectors as the target for

fitting decoding models with RSL. Predicted coordinates are then used to generate predicted

semantic distances between pairs of held-out stimuli. To understand the possible causes of

domain differences in prediction accuracy, we considered how well pairwise distances can be

reconstructed from the first three singular vectors and values computed from the true matrix with

a subset of items excluded. The goal was to assess whether the first three components capture

inter-items distances equally well for both domains or whether such distances are better

approximated for one domain than another.

1172   To this end we conducted the following analysis. We generated 10,000 random splits of

1173   the semantic norming data, each consisting of 90 training items and ten test items (five animate

1174   and five inanimate) as in the ECoG study. For each, we computed the SVD on the semantic

1175   distance matrix for only the items in the training set. We then projected test-set items into the

1176   resulting space by matrix multiplying each item's similarity with the training set items:

$$\widehat{C}_{q\times r} = S'_{q\times p} U_{p\times r} D_{r\times r}; S' = \left(S_{ij}\right)_{\substack{i\in test \\ j\in training}}$$

1178   Here $q = 10$ is the number of test set items, $p = 90$ is the number of training-set items,

$r = 3$ is the rank of the embedding, $\widehat{C}_{q\times r}$ is a matrix containing estimates coordinates for the test

items, S' is a matrix containing the true distances from test items to training items, and U and D

are matrices containing the singular vectors and values, respectively, computed the training

items. From the estimates coordinates in $\widehat{C}_{q\times r}$, the predicted similarity matrix can be obtained as

$\widehat{S}_{q\times q} = \widehat{C}D\widehat{C}^T$. To measure how well the true distances are captures by the SVD, we computed

correlations of lower-triangular values between S and $\widehat{S}$, either over all values at once or

correlating the animate-animate, inanimate-inanimate, and animate-inanimate similarity values

separately.

Figure S3 shows the average correlations for each selection of similarities over the

10,000 splits as bars with error bars reflecting the standard deviation over splits. The mean over

the 10 cross-validation splits used in the ECoG study are overlaid as points. Predicted similarities

that include or isolate between-category structure are most correlated with the true similarity

structure. Predicted within-category similarities are less correlated, with predictions for

inanimate items being less accurate than for animate items. In other words, a low-rank

approximation of the semantic similarity matrix best captures between-domain distances and

provides a better approximation of within-animate than within-inanimate semantic structure.

Thus, decoding models face an intrinsic disadvantage at capturing within-domain structure

generally, and within-inanimate structure specifically.

Figure S3. Correlation between true and reconstructed similarity matrices. Reconstructed similarity matrices are based on a SVD of a subset of the full similarity matrix expressing the pairwise similarities for 90 items, which is then used to reconstruct the similarities for the remaining 10 items as described in the text. This process was repeated 10,000 times with different 90/10 splits and each reconstruction was correlated with the corresponding true pairwise similarities. Bars show the average correlations over all similarities, just the between-category similarities (animate-inanimate), and just the within-category similarities (animate-animate and inanimate-inanimate). Error bars report the standard deviation of the means. The results for the specific 90/10 split used in the analysis of ECoG data reported in the main document are shown as black dots.

Appendix E: Correlation between predicted and full-rank semantic distances

In evaluating how well the RSL decoding models predict pairwise semantic similarities,

the main paper reports the correlation between predicted similarities and similarities

reconstructed directly from the three singular vectors computed from the "true" full-rank matrix.

We will refer to this as the *low-rank* similarity matrix. The low-rank similarity matrix represents

the best possible prediction, given that only three components of the true matrix were used to fit

the decoding model. Here we report correlations with the *full-rank* similarity matrix—the actual

pairwise similarities amongst feature vectors as described in the main text. The low-rank and

full-rank similarity matrices are very similar, $r = .94$, such that the low-rank similarity matrix

accounts for ~90% of the variance in the full-rank matrix. As one would expect given the high

correlation, **Figure S4** and **Figure 5** from the main document show the same pattern of results.

Filled circles indicate significance at Westfall-Young FWER corrected $\alpha = .05$.

Figure S4 Correlation between predicted semantic similarities and *full-rank* cosine similarities as computed from the feature vectors. These results are very similar to **Figure 5** in the main document which involves the *low-rank* similarity matrix, as reconstructed from the three semantic dimensions modeled in the primary analysis. The results are so similar because the first three components account for ~90% of the variance in the full-rank cosine similarity matrix. The interpretation is the same as **Figure 5**.

1209   **Appendix F: Temporal generalization profiles of models fit within moving windows**

1210   The model fit within a moving window can be used to decode target signal from the data

within all other moving windows, forming a temporal generalization profile forwards and

backwards through time. In Figure S5, each row in each panel is the temporal generalization

profile for one 100ms window. Colored points are significant with FDR-corrected p<.05,

correcting over the three panels in a single row (i.e., the multiple subsets relative to a shared

dependent variable). Profiles are shown for RSA-style paired-matrix correlations (Cosine

Similarities) and for correlations between model predictions and the target embedding along each

semantic component. Each analysis can be performed over all items or by restricting to within-

animate or within-inanimate similarities.

1219   Generalization is better at later time points, but some degree of reliable generalization is

1220   seen through time for most models that perform well on the window it was fit within for

1221   component 1 and the aggregate cosine similarities. However, this is not seen when decoding

1222   components 2 and 3. Models fit early in the epoch do not generalize to later time points, and

1223   models fit late in the epoch do not generalize to early in the epoch.

1224   The terms "early" and "late" are intentionally vague. We are not arguing for a qualitative,

1225   discrete shift in representational content at a particular point in time. If concepts encoded in the

1226   ATL follow a non-linear activation trajectory, as is often observed in deep network architectures,

1227   that is sufficient to make "early" and "late" representations importantly different while still

1228   conveying aspects of the target structure (Rogers et al., 2021).

Figure S5. Temporal generalization profiles for each model fit within a single 100ms-moving-window and tested on all windows. Colored points are significant with FDR-corrected p<.05, correcting over the three panels in a single row (i.e., the multiple subsets relative to a shared dependent variable). The first row shows the correlations between predicted similarity matrices and the target similarity matrix. Subsequent rows show the correlation between single predicted and target components.

1229

Appendix G: Anatomical distribution of decoding model weights across vATL

The decoding results reported in the main paper demonstrate that multi-dimensional

semantic structure can be decoded from LFPs recorded from the vATL, and that decoding the

second semantic dimension depends on regularization via the grOWL. This implies that local

neural populations do not independently encode each semantic dimension, but simultaneously

express multiple orthogonal components of the target semantic matrix. To evaluate whether this

is so, we examined the spatial distribution of weights across electrodes in the decoding models

predicting variation on the first via the second semantic dimensions for opening windows of size

200, 400, 600, 800, and 1000ms in the eight patients with electrodes implanted in the left

hemisphere. To obtain a single number at each electrode for each model (each component is

associated with a distinct model), the weight magnitudes (absolute values) were summed over

time. Because the number of electrodes and their placement varied across participants, we

projected these sums onto a standard MNI cortical surface and smoothed along the surface with a

4mm Gaussian kernel before averaging across participants. Points on the surface that are

associated with data from fewer than six participants are excluded from analysis. To determine

which sums are larger than expected by chance, the data for each participant within each window

was fit to 1,000 random row-wise permutations of the target structure. Each of these solutions

were projected onto the MNI surface as described above, resulting in 1,000 surface maps per

participant. Then we sampled a map from each participant to simulate one "experiment", and the

data were summed and averaged as above. This was repeated 10,000 times to obtain a group-

level null distribution (Stelzer et al., 2013).

Figure S6. Significant vertices on the standard MNI N27 surface reconstruction displayed with AFNI SUMA for eight patients with left lateralized language (confirmed with the WADA test). a) RSL model coefficients (multi-task linear regression with grOWL regularization) associated with points in MNI space were projected onto and smoothed along the surface with a 4mm Gaussian kernel, separately for dimensions 1 and 2. This was repeated for 10,000 group-level maps simulating the null distribution at each vertex by permutation. Only points on the surface where data from 6 or more patients is available are considered; vertices meeting this criterion are contained within the red contour. Vertices with average weight magnitude larger than 9,500 of the 10,000 group-level values in the permutation distribution for that vertex are shown: points that meet these criteria for dimension 1 are shown in yellow, for dimension 2 are shown in blue, and for both are shown in green. b) Number of electrodes contributing to the data at each vertex after applying a 4mm Gaussian kernel. c) Tabulation of significant vertices.

Figure S6a displays the points on the cortical surface where the real average is larger

than 9,500 of the values in this null distribution. Points on the surface that are associated with

large model weights for the first component (but not the second) are shaded yellow; points that

are associated with the second component (but not the first) are shown in blue. Points on the

surface that are associated with large weights for both components in the same model are shown

with green. Substantial overlap is observed in all windows, with overlap increasing with window

length (**Figure S6c**). Furthermore, both semantic dimensions are encoded across the vATL with

little functional localization.