1 **Title:** TRPV1-mediated sonogenetic neuromodulation of motor cortex in freely moving mice

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22 Abstract

Background: Noninvasive and cell-type-specific neuromodulation tools are critically needed for probing intact brain function. Sonogenetics for noninvasive activation of neurons engineered to express thermosensitive transient receptor potential vanilloid 1 (TRPV1) by transcranial focused ultrasound (FUS) was recently developed to address this need. However, using TRPV1-mediated sonogenetics to evoke behavior by targeting the cortex is challenged by its proximity to the skull due to high skull absorption of ultrasound and increased risks of thermal-induced tissue damage.

30 **Objective:** This study evaluated the feasibility and safety of TRPV1-mediated sonogenetics
 31 in targeting the motor cortex to modulate the locomotor behavior of freely moving mice.

Methods: Adeno-associated virus was delivered to the mouse motor cortex via intracranial injection to express TRPV1 in excitatory neurons. A wearable FUS device was installed on the mouse head after a month to control neuronal activity by activating virally expressed TRPV1 through FUS sonication at different acoustic pressures. Immunohistochemistry staining of *ex vivo* brain slices was performed to verify neuron activation and evaluate safety.

Results: TRPV1-mediated sonogenetic stimulation at 0.7 MPa successfully evoked rotational behavior in the direction contralateral to the stimulation site, activated cortical neurons as indicated by the upregulation of c-Fos, and did not induce significant changes in inflammatory or apoptotic markers (GFAP, Iba1, and Caspase-3). Sonogenetic stimulation of TRPV1 mice at a higher acoustic pressure, 1.1 MPa, induced significant changes in motor behavior and upregulation of c-Fos compared with FUS sonication of naïve mice at 1.1 MPa. However, signs of damage at the meninges were observed at 1.1 MPa.

45 Conclusions: TRPV1-mediated sonogenetics can achieve effective and safe
46 neuromodulation at the cortex with carefully selected FUS parameters. These findings
47 expand the application of this technique to include superficial brain targets.

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49 Keywords: TRPV1, sonogenetics, motor cortex, ultrasound, behavior, neuromodulation

50 Introduction

51 The evolution of brain neuromodulation tools has provided unprecedented opportunities to 52 probe neural circuits, understand brain function, and develop new treatment strategies for 53 brain diseases. Transcranial neuromodulation tools, such as direct current, magnetic 54 stimulation, and ultrasound stimulation, offer noninvasive ways to stimulate the brain and 55 have contributed to the understanding of brain function [1,2]. The lack of cell-type specificity 56 in these tools, however, limits their utility in understanding the brain at cellular resolution. 57 Genetic-based neuromodulation tools, such as optogenetics and chemogenetics, encode 58 stimulus-sensitive probes into a defined neuron population and have transformed 59 fundamental neuroscience research [3,4]. Each method, however, suffers from its own 60 limitations. Most commonly, optogenetics requires the invasive implantation of optical probes 61 to deliver light to opsin-encoding neurons, limiting the ability to study the brain without the 62 risk of ischemia and inflammation. Noninvasive optogenetics modulates the activity of opsin-63 encoding neurons via transcranial illumination, but light scattering in brain tissue limits its 64 depth penetration in large animal models [5]. On the other hand, chemogenetics 65 noninvasively activates neurons encoding designer receptors exclusively activated by 66 designer drugs (DREADDs) via minimally-invasive systemic delivery of designer drugs, but 67 the long residence time of circulating drugs sacrifices the temporal resolution of this 68 technique. There is a clear need for techniques that can facilitate noninvasive, cell-type 69 specific neuromodulation with high spatiotemporal resolution and the potential to be scaled 70 up to large animals and humans.

71

Sonogenetics has great potential to fulfill this gap. Analogous to other genetic-based neuromodulation tools, sonogenetics uses focused ultrasound (FUS) to modulate the activity of neurons encoding ultrasound-sensitive actuators [6]. Unlike other stimulation modalities (e.g., light, electricity, and magnetic fields), FUS can achieve noninvasive, spatiotemporally precise targeting of any brain region in small animals [7], large animals [2], and even

77 humans [8]. Sonogenetics was first demonstrated in 2015 using C. elegans, in which 78 mechanosensitive TRP-4 ion channel expression in neurons in combination with 79 microbubbles evoked behavioral changes upon ultrasound stimulation [9]. Since the first 80 demonstration of sonogenetics, many other mechanosensitive ion channels and proteins 81 have been proposed to sensitize cells to ultrasound stimulation in vitro, including TREK1, 82 TREK2, TRAAK [10], MscL [11], Piezo1 [12], MEC-4 [13], prestin [14], TRPA1 [15], TRPC1, 83 TRPP2, and TRPM4 [16]. Recently, multiple studies demonstrated the feasibility of 84 sonogenetics to modulate mouse behavior in vivo using ultrasound-sensitive probes such as 85 prestin [17], MscL G22S [18], and TRPA1 [19].

86

87 Ultrasound propagation in tissue can generate not only mechanical effects but also thermal 88 effects. The transient receptor potential vanilloid 1 (TRPV1) ion channel is extremely 89 sensitive to temperature and has a thermal activation threshold of approximately 42°C, 90 which is only a few degrees above the physiological body temperature of many mammals 91 [20]. Such an activation temperature allows TRPV1 to be closed at the physiological body 92 temperature and open upon sufficient heating to \sim 42°C. Because of these unique features, 93 TRPV1 has been used to develop genetics-based neuromodulation techniques, such as 94 magneto-thermogenetics [21,22] and photothermal genetics [23]. TRPV1-mediated 95 sonogenetics was recently developed to achieve noninvasive, cell-type specific 96 neuromodulation. Our previous study demonstrated that TRPV1 is an ultrasound-sensitive 97 actuator, and that TRPV1-mediated sonogenetics can control the motor behavior of freely 98 moving mice by targeting a deep brain region, the striatum [24]. However, the capability of 99 TRPV1-mediated sonogenetics in controlling mouse behavior by targeting the superficial 100 brain area has not been demonstrated. Targeting superficial brain regions is challenging for 101 TRPV1-mediated sonogenetics because the high absorption of ultrasound in the skull could 102 increase the risk of overheating the cortex area directly underneath the skull [25,26]. This 103 could increase the risk of undesirable neuromodulatory effects associated with heating and 104 potential tissue damage when the temperature is high. Therefore, the objective of the current

- 105 study was to assess the capability of TRPV1-mediated sonogenetics in evoking mouse
- 106 motor behavior by targeting a superficial brain target the motor cortex.

107 Materials and methods

108 **Stereotaxic injection of virus**

109 All animal procedures were performed under a protocol approved by the Washington 110 University in St. Louis Institutional Animal Care and Use Committee (IACUC). C57/BL6 mice 111 (female, 6-8 weeks old) were purchased from Charles River and housed in an animal facility 112 under a 12 hour light-dark cycle. Adeno-associated viruses (AAV) were introduced to 113 CaMKII-expressing neurons of the M2 cortex to overexpress TRPV1 ion channel. All 114 surgeries were conducted under aseptic conditions. Mice were anesthetized with 2% 115 isoflurane in oxygen at a rate of 1.0 L/min in an anesthetic chamber for induction and 1.5% 116 isoflurane for maintaining anesthesia. Anesthetized mice were then fixed onto a stereotaxic 117 frame (Kopf Instruments) using a bite bar and ear bars. Buprenorphine SR (1.0 mg/kg) was 118 administered subcutaneously for pre-operative and post-operative pain management. The 119 head was shaved and was rubbed with skin disinfectant (Hibiclens). An incision was made 120 on the scalp, the skin was retracted, and the periosteum was removed. A small hole was 121 drilled through the skull (-1.0 mm ML, +2.5 mm AP, -1.0 mm DV), and a micro-injector 122 (Nanoject II, Drummond Scientific) was inserted into the motor cortex. 1200 nL of TRPV1 123 virus (1.4e12 vg/mL) was introduced at a rate of 64 nL/min. 1000 nL of control virus (3.2e12 124 vg/mL) was introduced to approximately match the viral genome copy numbers delivered to 125 the motor cortex. After injection, the micro-injector was slowly removed, the hole was filled 126 with bone wax, and the scalp was sutured. Mice were housed for at least 4 weeks to 127 facilitate sufficient virus expression before further treatments were conducted.

128

129 Wearable FUS device

A wearable FUS device was used to stimulate the motor cortex of freely moving mice, and the design is described in the first report of TRPV1-mediated sonogenetics [24]. In brief, the wearable FUS device consisted of two parts: a FUS transducer and a base plate. The FUS transducer was made of a lead zirconate titanate (PZT) ceramic resonator (DL-43, DeL

Piezo Specialties) encapsulated by a 3D-printed housing. The PZT ceramic resonated at a frequency of 1.5 MHz and had an aperture of 10 mm and a radius of curvature of 10 mm. The wearable FUS transducer was plugged into the base plate, a 3D printed circular adapter attached to the mouse skull. When the FUS transducer was plugged into the base plate, the wearable FUS device was stabilized on the mouse head.

139

Each component of the wearable FUS device was specifically designed to target the motor cortex. The base plate was designed with a hole in its geometric center to facilitate the alignment of base plate to the medial-lateral and anterior-posterior coordinates of the motor cortex. The height of the FUS transducer housing was designed to align the FUS focus to the dorsal-ventral coordinates of the motor cortex. The entire wearable FUS device was calibrated by a hydrophone (HGL-200, Onda). The full width half-maximum of the FUS focal region was approximately 0.9 mm and 2.5 mm in the lateral and axial directions, respectively.

147

148 Attachment of FUS transducer base plate to the mouse skull

149 Four to five weeks after virus injection, mice were again anesthetized with isoflurane (2% for 150 induction, 1.5% for maintenance), fixed in a stereotaxic frame, and subcutaneously 151 administered with Buprenorphine SR (1.0 mg/kg). A piece of the scalp was removed, the 152 periosteum was removed, and the drilled hole from the intracranial injection of AAV was 153 identified and accentuated with a marker. The custom designed base plate was 3D-printed 154 and glued onto the skull using dental adhesives (Metabond) with the center of the base plate 155 aligned to the pre-drilled hole. The mice were housed for a week to facilitate sufficient 156 recovery before performing behavior experiments.

157

158 **FUS stimulation with behavior recording**

Prior to the behavior test, mice were adapted to the behavior recording environment by placing the mouse in the behavior testing arena with the power amplifier turned on. During the behavior recording, mice were lightly anesthetized with isoflurane (1% induction and

maintenance). The base plate on the mouse and the wearable ultrasound transducer were both sufficiently filled with degassed ultrasound gel (Aquasonics). The wearable transducer was then securely plugged into the base plate of the mouse, and the mouse was then placed in a circular arena on a heating pad for 30 min to allow the mouse body temperature to recover from any possible anesthesia effects. The heating pad was then removed, and the mouse was allowed to habituate for 15 min in the actual behavior test arena.

168

169 During the recording period, focused ultrasound was applied at a frequency of 1.5 MHz, duty 170 cycle of 40%, PRF of 10 Hz, and 15 s total sonication duration with 185 s inter-stimulation 171 interval for a total of 5 stimulations. The onset and offset of the ultrasound pulse was 172 smoothed to avoid possible auditory effects [27]. The acoustic pressures used in the study 173 were 0, 0.7, and 1.1 MPa to investigate the effect of pressure on locomotor behavior 174 outcomes. Custom MATLAB software was used to control when ultrasound was applied via 175 an Arduino Uno. A red LED attached to the Arduino Uno would turn on when ultrasound was 176 applied to precisely synchronize mouse behavior to each focused ultrasound stimulation. In 177 each group, mice were given five consecutive focused ultrasound stimulations at one 178 pressure.

179

180 Behavioral analysis

Mice were recorded using a camera (Logitech C920X, 30 fps) before, during, and after each focused ultrasound stimulation. During the recording session, each video is simultaneously processed using Bonsai to quantify the positional coordinates and the angular orientation of the mice. After conducting recordings, data were processed using a custom MATLAB script to compute the average angular velocities upon FUS stimulation at different acoustic pressures.

187

188 Immunohistological analysis

189 Approximately 90 minutes after the last FUS stimulation, TRPV1- and TRPV1+ mice from 190 each acoustic pressure stimulation group were sacrificed via transcardial perfusion with 1x 191 PBS solution for the evaluation of TRPV1 expression, c-Fos expression, and safety of 192 sonogenetics via inflammatory and apoptotic markers (GFAP, Iba1, and Caspase-3). A 193 sacrifice time of 90 minutes post stimulation was chosen to visualize the peak expression of 194 c-Fos [28]. This time was also suitable to visualize any rapid recruitment of inflammatory and 195 apoptotic markers at the FUS stimulation site [29]. The brains were fixed in 4% w/v 196 paraformaldehyde in 1x PBS solution overnight and were transferred to 15% and 30% w/v 197 sucrose in 1x PBS for the following two days, respectively. The brain tissue was embedded 198 in a cryomold with Optimal Cutting Temperature medium (Scigen) to generate 10 µm thick 199 coronal brain slices affixed on a glass slide.

200

201 For evaluation of TRPV1 and c-Fos expression, slides with brain tissue were stained with 202 anti-TRPV1 antibody (Novus Biologicals, 1:200), anti-c-Fos antibody (Cell Signaling, 1:1000), 203 and Nissl stain (Invitrogen, 1:100). TRPV1 and c-Fos were visualized using Alexa Fluor 594 204 and 488 secondary antibody (Jackson ImmunoResearch, 1:400), respectively. For cellular 205 safety evaluation, slides with brain tissue were stained with anti-GFAP antibody (Abcam, 206 1:1000), anti-Iba1 antibody (Wako, 1:1000), or anti-Caspase-3 antibody (Cell Signaling, 207 1:2500), as well as DAPI mounting medium (Vector). GFAP, Iba1, and Caspase-3 cells were 208 visualized using Alexa Fluor 488 secondary antibody (Jackson ImmunoResearch, 1:400). 209 Cell counts were computed in the motor cortex using QuPath (University of Edinburgh). The 210 viral spread was quantified by drawing a region that encapsulated all the TRPV1+ neurons. 211 TRPV1+ and c-Fos+ neuron cell densities were calculated by counting the total number of 212 positively stained Nissl cells over the motor cortex region. GFAP, Iba1, and Caspase-3 cell 213 counts were calculated by counting the total number of positively-stained DAPI cells over the 214 motor cortex region.

- 215
- 216 Statistics

- 217 Statistical tests were conducted using GraphPad. Data were analyzed using either a two-
- tailed t-test or repeated measures ANOVA with either Bonferroni's post-hoc test (to compare
- row- and column-wise groups) or Dunnett's post-hoc test (to compare to a control group).
- 220 Statistical differences were considered significant whenever $p \square < \square 0.05$. All graphs presented
- results as the mean $\exists \pm \exists$ standard error of the mean (SEM).

222 Results

223 We intracranially injected adeno-associated virus (AAV) to the mouse motor cortex (M2) to 224 express TRPV1 primarily in excitatory neurons under the CaMKII promoter (Fig. 1a). These 225 mice are referred to as TRPV1+ mice. Control mice were injected with TRPV1- virus, 226 referred to as TRPV1- mice. After sufficient virus expression, a wearable FUS transducer 227 was attached to the mouse head. Mouse locomotion was assessed before, during, and after 228 FUS sonication in an open-field behavior test arena. FUS sonication was targeted at the 229 motor cortex using the same coordinates as the virus injection by mechanically aligning the 230 FUS device to the craniotomy from the virus injection. FUS was applied with a center 231 frequency of 1.5 MHz, a pulse repetition frequency (PRF) of 10 Hz, a duty cycle (DC) of 40%, 232 acoustic pressures of 0.7 and 1.1 MPa, and a burst duration (BD) of 15 s with an inter-233 stimulation interval (ISI) of 185 s for a total of five stimulations (Fig. 1b). Mice were 234 sacrificed after the behavior test to evaluate the expression of TRPV1, the activation of 235 neurons (c-Fos), and safety of sonogenetics.

236

237 Characterization of exogenous TRPV1 expression in the motor cortex

238 We first describe the virus expression level of TRPV1 in the motor cortex. The brains of 239 TRPV1+ mice were harvested, sectioned, and co-stained with anti-TRPV1 antibody and 240 Nissl to evaluate the expression profile of TRPV1 in cortical neurons of the motor cortex. A 241 representative brain slice of a TRPV1+ mouse illustrated that TRPV1 expression was 242 primarily confined to the motor cortex (Fig. 2a). As expected, the contralateral non-injection 243 site did not express any TRPV1 in cortical neurons of the motor cortex. The viral spread of 244 TRPV1 in the cortex was $1.06 \pm 0.07 \text{ mm}^2$, and the density of neurons in the motor cortex 245 that were virally transduced to express TRPV1 was 66.7 ± 4.0 cells/mm² (Fig. 2b-c). The 246 proportion of neurons in the motor cortex that expressed TRPV1 cells was $5.16 \pm 0.43\%$ 247 (Fig. 2d). Higher magnification of the virus transduction region showed that TRPV1 248 expression was largely confined to neurons, in which 83.4 ± 3.0% of the cells transfected

with TRPV1 were neurons (Fig. 2e). These data demonstrate the feasibility of exogenous
TRPV1 expression in the motor cortex region and lay the foundation to facilitate TRPV1-

- 251 mediated sonogenetic control of motor cortex behaviors.
- 252

TRPV1-mediated sonogenetic neuromodulation within the motor cortex alters locomotor behavior

255 We recorded the locomotor behavior of TRPV1- and TRPV1+ mice with the application of 256 FUS at the motor cortex to assess the ability of TRPV1-mediated sonogenetics in 257 modulating locomotor behavior. Representative locomotor behavior of TRPV1- and TRPV1+ 258 mice with and without FUS are shown as position traces (Fig. 3a; TRPV1-, Movie S1; 259 TRPV1+, Movie S2). FUS sonication at 0.7 MPa did not evoke considerable motion in 260 TRPV1- mice compared to that before FUS. In TRPV1+ mice, however, FUS stimulation did 261 evoke rotational behavior around the behavior testing arena, which was not observed before 262 FUS. During the FUS sonication periods (shown by the highlighted yellow bars), TRPV1+ 263 mice displayed rotational behavior indicated by changes in angular displacement and 264 angular velocity (Fig. 3b, 3c). In contrast, TRPV1- mice did not demonstrate any rotational 265 bias upon FUS sonication.

266

267 We then compared the average angular velocities of TRPV1- and TRPV1+ mice with FUS at 268 acoustic pressures of 0.7 and 1.1 MPa. In the TRPV1+ mice group, FUS stimulation at 0.7 269 MPa evoked a significant increase in angular velocity $(0.86 \pm 0.23 \text{ rev/min})$ compared to the 270 sham stimulation at 0 MPa (-0.22 ± 0.25 rev/min), indicating that TRPV1+ mice displayed a 271 preference to rotate in the direction contralateral to the stimulation site (Fig. 4; ~4-fold 272 increase, p = 0.026, two-way repeated measures ANOVA with Bonferroni's post-hoc test). In 273 contrast, FUS stimulation at 0.7 MPa did not evoke any significant angular velocity changes 274 in the TRPV1- mice group relative to the sham stimulation (0.7 MPa: -0.20 ± 0.31 rev/min; 0 275 MPa: -0.17 ± 0.21 rev/min). These findings indicate that TRPV1-mediated sonogenetics at 276 0.7 MPa can achieve circuit-specific control of locomotor behaviors in the motor cortex.

277 Increasing the acoustic pressure to 1.1 MPa did not evoke significant changes in angular 278 velocity compared to the sham stimulation at 0 MPa in TRPV1+ mice (1.1 MPa: 0.36 ± 0.53 279 rev/min). However, sonogenetics stimulation at 1.1 MPa of TRPV1+ mice achieved a 280 significantly higher angular velocity than that obtained by FUS sonication at 1.1 MPa of 281 TRPV1- mice (p = 0.036). Although not statistically significant, FUS sonication at 1.1 MPa of 282 TRPV1- mice evoked an increase in the average angular velocity in the ipsilateral direction (-283 0.88 ± 0.36 rev/min) compared with those at 0 MPa and 0.7 MPa. These findings suggest 284 that FUS stimulation at 1.1 MPa alone (without TRPV1) potentially induced neuromodulation 285 effects and generated a confounding impact on TRPV1-mediated sonogenetics at this high-286 pressure level.

287

288 TRPV1-mediated sonogenetics activates cortical neurons on the cellular level

289 To provide a secondary readout for successful modulation of the motor cortex using 290 sonogenetics, we sacrificed the mice 90 minutes after the final stimulation and used 291 immunohistochemical staining to analyze c-Fos expression levels of TRPV1+ and TRPV1-292 mice. Representative fluorescent images of TRPV1- and TRPV1+ brains stimulated at 293 different acoustic pressures demonstrate that sonication at both 0.7 MPa and 1.1 MPa 294 elicited greater c-Fos expression levels in the motor cortex of TRPV1+ mice (Fig. 5a). Group 295 analysis found that TRPV1+ mice showed enhancement in the number of c-Fos cells at both 296 0.7 MPa (231.5 ± 58.3 cells/mm²) and 1.1 MPa (332.1 ± 74.2 cells/mm²) compared to the 297 unstimulated side (89.4 ± 22.2 cells/mm²), indicating activation of neurons in the motor 298 cortex (Fig. 5b; 0.7 MPa: ~2.6-fold change, p = 0.011; 1.1 MPa: ~3.7-fold change, p < 299 0.0001; two-way ANOVA with Bonferroni's post-hoc test). On the other hand, FUS 300 stimulation at 0.7 MPa and 1.1 MPa did not evoke significant enhancements in c-Fos 301 expression in TRPV1- mice (0 MPa: 70.1 \pm 19.1 cells/mm²; 0.7 MPa: 51.8 \pm 21.8 cells/mm²; 302 1.1 MPa: 144.5 \pm 50.4 cells/mm²). While there is a slight potential increase in c-Fos 303 expression in TRPV1- mice from FUS alone at 1.1 MPa compared to the unstimulated 304 control, this relationship was not statistically significant (p = 0.34). These data demonstrate

305 the ability of TRPV1-mediated sonogenetics to activate motor cortex neurons at the cellular

306 level at both 0.7 MPa and 1.1 MPa.

307

308 Inflammatory and apoptotic responses in the brain are not engaged by TRPV1-

309 mediated sonogenetics

310 Gross pathology of the mice skull and brain stimulated at 0.7 MPa showed no signs of 311 damage (Fig. 6a). In contrast, bleeding was consistently observed in the meninges between 312 the skull and the brain at 1.1 MPa. Furthermore, we used Nissl to stain for signs of neuronal 313 damage, GFAP and Iba1 to stain for signs of inflammation, and Caspase-3 to stain for signs 314 of apoptosis (Fig. 6b). Using the non-injection and non-stimulated side of both TRPV1+ and 315 TRPV1- mice as the control, there were no significant differences in any of the protein 316 marker expression levels in the mouse brain at 0.7 MPa or 1.1 MPa (Fig. 6c; one-way 317 repeated measures ANOVA with Dunnett's post-hoc test). Both gross pathology and 318 immunohistological analysis of inflammatory and apoptotic markers showed that TRPV1-319 mediated sonogenetics at 0.7 MPa enables safe neuromodulation, while damage at the 320 meninges was associated with sonogenetics at 1.1 MPa.

322 Discussion

323 Sonogenetics is a rapidly emerging technique that enables noninvasive, cell-type specific 324 neuromodulation with high spatiotemporal resolution. This study demonstrates the capability 325 of TRPV1-mediated sonogenetics to modulate behavior in freely moving mice.

326

327 Previous studies have reported sonogenetic-enabled neuromodulation in mice by activating 328 mechanosensitive ion channels and proteins, such as prestin [17], MscL G22S [18], and 329 TRPA1 [19], using FUS-induced mechanical effects. They observed neuron activation based 330 on c-Fos staining, as well as motor responses in head-fixed anesthetized mice based on 331 electromyography, but did not report induction of real-time behavior modulation in freely 332 moving mice. Different from these studies, the current study used thermosensitive ion 333 channel TRPV1-mediated sonogenetics and achieved successful behavior modulation in 334 freely moving mice. Our previous study demonstrated successful locomotor behavior 335 modulation by TRPV1-mediated sonogenetics in freely moving mice by targeting a deep 336 brain region, the striatum [24]. Here we demonstrated that this technique could modulate 337 locomotor behaviors via a superficial brain target (motor cortex), expanding the application 338 of TRPV1-mediated sonogenetics to include both superficial and deep brain targets.

339

340 Previous studies have also reported successful neuromodulation using TRPV1-mediated 341 neuromodulation via combining TRPV1 with different external stimulation modalities. 342 TRPV1-mediated magnetothermal-genetics targeting both superficial and deep brain targets 343 were previously reported [21,22]; however, magnetic nanoparticles need to be injected into 344 the brain to convert energy from an alternating magnetic field to heat for TRPV1 activation. 345 Recently, TRPV1-mediated photothermal genetic stimulation was reported, which combines 346 an injection of nanoparticles with near-infrared light to generate heat for TRPV1 activation 347 [23]. TRPV1-mediated magnetothermal and photothermal genetic modulation of the motor 348 cortex induced increases in the angular speed of freely moving mice in the contralateral direction, which was consistent with the results of this study at 0.7 MPa sonication. However, both existing techniques require an additional component of "energy-converting" nanoparticles that were directly injected into brain tissue. The injection process poses inflammation and ischemia risks, and the presence of nanoparticles in the brain possesses immunogenic and biocompatibility concerns. Since FUS-mediated heating does not require the injection of nanoparticles, it provides a powerful alternative approach to achieving TRPV1-mediated genetic neuromodulation.

356

357 We show that TRPV1-mediated sonogenetics successfully evoked motor behavior by 358 targeting the superficial brain target with carefully selected ultrasound parameters. 359 Ultrasound parameters must be selected to achieve successful behavior control without 360 causing any detectable tissue damage. Based on behavior, c-Fos, and safety analyses, 361 TRPV1-mediated sonogenetics at 0.7 MPa met this requirement. However, increasing the 362 pressure to 1.1 MPa did not evoke statistically significant changes in angular velocity in 363 TRPV1+ mice relative to the sham sonication at 0 MPa, but evoked significant changes 364 compared to FUS sonication of TRPV1- mice at 1.1 MPa. FUS sonication at 1.1 MPa in 365 TRPV1- mice showed a trend, although not significant, to evoke ipsilateral rotations. These 366 findings suggested that FUS stimulation at 1.1 MPa alone could impact animal behavior. It 367 was interesting to find that damage to the meninges was observed at 1.1 MPa, although no 368 damage to the brain tissue was clearly detected. Damage to the meninges was due to its 369 proximity to the skull. The high skull absorption of ultrasound at 1.1 MPa caused thermal-370 induced damage to the meninges. Therefore, ultrasound parameter selection must be 371 carefully selected when performing TRPV1-mediated sonogenetics to achieve effective and 372 safe neuromodulation.

374 Conclusion

- 375 In conclusion, our findings demonstrated the feasibility and safety of using TRPV1-mediated
- 376 sonogenetics to modulate locomotor behaviors by targeting the motor cortex. Combined with
- 377 our previous report on TRPV1-mediated sonogenetics for behavior modulation by targeting
- 378 the deep brain region, our present study indicates that this technique can facilitate
- neuromodulation at the whole depth of the mouse brain.

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385

386 **Conflict of interest:** Authors report no conflict of interest.

- 388 **Data statement:** The data that from this study are available from the corresponding author
- 389 upon reasonable request.

390 References

- 391 [1] Wagner T, Valero-Cabre A, Pascual-Leone A. Noninvasive human brain stimulation.
- 392 Annu Rev Biomed Eng 2007;9:527–65.
- 393 https://doi.org/10.1146/annurev.bioeng.9.061206.133100.
- 394 [2] Folloni D, Verhagen L, Mars RB, Fouragnan E, Constans C, Aubry JF, et al.
- 395 Manipulation of Subcortical and Deep Cortical Activity in the Primate Brain Using
- 396 Transcranial Focused Ultrasound Stimulation. Neuron 2019;101:1109-1116.e5.
- 397 https://doi.org/10.1016/j.neuron.2019.01.019.
- 398 [3] Fenno L, Yizhar O, Deisseroth K. The development and application of optogenetics.
- Annu Rev Neurosci 2011;34:389–412. https://doi.org/10.1146/annurev-neuro-061010113817.
- 401 [4] Sternson SM, Roth BL. Chemogenetic tools to interrogate brain functions. Annu Rev
 402 Neurosci 2014;37:387–407. https://doi.org/10.1146/annurev-neuro-071013-014048.
- 403 [5] Chen R, Gore F, Nguyen QA, Ramakrishnan C, Patel S, Kim SH, et al. Deep brain
- 404 optogenetics without intracranial surgery. Nat Biotechnol 2021;39:161–4.
- 405 https://doi.org/10.1038/s41587-020-0679-9.
- 406 [6] Rabut C, Yoo S, Hurt RC, Jin Z, Li H, Guo H, et al. Ultrasound Technologies for
- 407 Imaging and Modulating Neural Activity. Neuron 2020;108:93–110.
- 408 https://doi.org/10.1016/j.neuron.2020.09.003.
- 409 [7] Tufail Y, Matyushov A, Baldwin N, Tauchmann ML, Georges J, Yoshihiro A, et al.
- 410 Transcranial Pulsed Ultrasound Stimulates Intact Brain Circuits. Neuron 2010;66:681–
- 411 94. https://doi.org/10.1016/j.neuron.2010.05.008.
- 412 [8] Legon W, Sato TF, Opitz A, Mueller J, Barbour A, Williams A, et al. Transcranial
- 413 focused ultrasound modulates the activity of primary somatosensory cortex in humans.
- 414 Nat Neurosci 2014;17:322–9. https://doi.org/10.1038/nn.3620.
- 415 [9] Ibsen S, Tong A, Schutt C, Esener S, Chalasani SH. Sonogenetics is a non-invasive
- 416 approach to activating neurons in Caenorhabditis elegans. Nat Commun 2015.

417 https://doi.org/10.1038/ncomms9264.

- 418 [10] Kubanek J, Shi J, Marsh J, Chen D, Deng C, Cui J. Ultrasound modulates ion channel
 419 currents. Sci Rep 2016. https://doi.org/10.1038/srep24170.
- 420 [11] Ye J, Tang S, Meng L, Li X, Wen X, Chen S, et al. Ultrasonic Control of Neural
- 421 Activity through Activation of the Mechanosensitive Channel MscL. Nano Lett
- 422 2018;18:4148–55. https://doi.org/10.1021/acs.nanolett.8b00935.
- 423 [12] Qiu Z, Guo J, Kala S, Zhu J, Xian Q, Qiu W, et al. The Mechanosensitive Ion Channel
- 424 Piezo1 Significantly Mediates In Vitro Ultrasonic Stimulation of Neurons. IScience
- 425 2019. https://doi.org/10.1016/j.isci.2019.10.037.
- 426 [13] Kubanek J, Shukla P, Das A, Baccus SA, Goodman MB. Ultrasound elicits behavioral
- 427 responses through mechanical effects on neurons and ion channels in a simple
- 428 nervous system. J Neurosci 2018. https://doi.org/10.1523/JNEUROSCI.1458-17.2018.
- 429 [14] Huang YS, Fan CH, Hsu N, Chiu NH, Wu CY, Chang CY, et al. Sonogenetic
- 430 Modulation of Cellular Activities Using an Engineered Auditory-Sensing Protein. Nano
 431 Lett 2020;20:1089–100. https://doi.org/10.1021/acs.nanolett.9b04373.
- 432 [15] Oh SJ, Lee JM, Kim HB, Lee J, Han S, Bae JY, et al. Ultrasonic Neuromodulation via
 433 Astrocytic TRPA1. Curr Biol 2019;29:3386-3401.e8.
- 434 https://doi.org/10.1016/j.cub.2019.08.021.
- 435 [16] Yoo S, Mittelstein D, Hurt R, Lacroix J, Shapiro M. Focused ultrasound excites
- 436 neurons via mechanosensitive calcium accumulation and ion channel amplification
- 437 2020. https://doi.org/10.1101/2020.05.19.101196.
- 438 [17] Fan CH, Wei KC, Chiu NH, Liao EC, Wang HC, Wu RY, et al. Sonogenetic-Based
- 439 Neuromodulation for the Amelioration of Parkinson's Disease. Nano Lett
- 440 2021;21:5967–76. https://doi.org/10.1021/acs.nanolett.1c00886.
- 441 [18] Qiu Z, Kala S, Guo J, Xian Q, Zhu J, Zhu T, et al. Targeted Neurostimulation in
- 442 Mouse Brains with Non-invasive Ultrasound. Cell Rep 2020;32.
- 443 https://doi.org/10.1016/j.celrep.2020.108033.
- 444 [19] Duque M, Lee-Kubli CA, Tufail Y, Magaram U, Patel J, Chakraborty A, et al.

- 445 Sonogenetic control of mammalian cells using exogenous Transient Receptor
- 446 Potential A1 channels. Nat Commun 2022;13. https://doi.org/10.1038/s41467-022-
- 447 **28205-y**.
- 448 [20] Dhaka A, Viswanath V, Patapoutian A. TRP ion channels and temperature sensation.
- 449 Annu Rev Neurosci 2006;29:135–61.
- 450 https://doi.org/10.1146/annurev.neuro.29.051605.112958.
- 451 [21] Chen R, Romero G, Christiansen MG, Mohr A, Anikeeva P. Wireless magnetothermal
 452 deep brain stimulation. Science (80-) 2015;347:1477–80.
- 453 https://doi.org/10.1126/science.1261821.
- 454 [22] Munshi R, Qadri SM, Zhang Q, Rubio IC, del Pino P, Pralle A. Magnetothermal
- 455 genetic deep brain stimulation of motor behaviors in awake, freely moving mice. Elife
- 456 2017;6. https://doi.org/10.7554/eLife.27069.
- 457 [23] Wu X, Jiang Y, Rommelfanger NJ, Yang F, Zhou Q, Yin R, et al. Tether-free
- 458 photothermal deep-brain stimulation in freely behaving mice via wide-field illumination
- in the near-infrared-II window. Nat Biomed Eng 2022;6:754–70.
- 460 https://doi.org/10.1038/s41551-022-00862-w.
- 461 [24] Yang Y, Pacia CP, Ye D, Zhu L, Baek H, Yue Y, et al. Sonothermogenetics for
- 462 noninvasive and cell-type specific deep brain neuromodulation. Brain Stimul 2021;0.
 463 https://doi.org/10.1016/j.brs.2021.04.021.
- 464 [25] Hynynen K, McDannold N, Clement G, Jolesz FA, Zadicario E, Killiany R, et al. Pre-
- 465 clinical testing of a phased array ultrasound system for MRI-guided noninvasive
- 466 surgery of the brain-A primate study. Eur J Radiol 2006;59:149–56.
- 467 https://doi.org/10.1016/j.ejrad.2006.04.007.
- 468 [26] Pinton G, Aubry JF, Bossy E, Muller M, Pernot M, Tanter M. Attenuation, scattering,
- and absorption of ultrasound in the skull bone. Med Phys 2012;39:299–307.
- 470 https://doi.org/10.1118/1.3668316.
- 471 [27] Mohammadjavadi M, Ye PP, Xia A, Brown J, Popelka G, Pauly KB. Elimination of
- 472 peripheral auditory pathway activation does not affect motor responses from

- 473 ultrasound neuromodulation. Brain Stimul 2019;12:901–10.
- 474 https://doi.org/10.1016/j.brs.2019.03.005.
- 475 [28] Kovács KJ. c-Fos as a transcription factor: A stressful (re)view from a functional map.
- 476 Neurochem Int 1998;33:287–97. https://doi.org/10.1016/S0197-0186(98)00023-0.
- 477 [29] Damisah EC, Hill RA, Rai A, Chen F, Rothlin C V., Ghosh S, et al. Astrocytes and
- 478 microglia play orchestrated roles and respect phagocytic territories during neuronal
- 479 corpse removal in vivo. Sci Adv 2020;6:1–13. https://doi.org/10.1126/sciadv.aba3239.

480

482 Figure Captions

483 Fig. 1. Experimental setup. (a) Experimental timeline. The study begins with intracranial 484 injection of adeno-associated virus encoding TRPV1 (TRPV1+ mice). Control mice were 485 injected with a control viral vector (TRPV1- mice). After 4-5 weeks, a wearable FUS device 486 was installed onto the mouse skull to target the same location where the viral vectors were 487 injected. The stimulation apparatus consists of a computer, function generator, and power 488 amplifier to apply FUS to the wearable FUS device. Approximately 90 minutes after the final 489 stimulation, mice brains were harvested for c-Fos and safety analyses. (b) Schematic of the 490 ultrasound waveform used during the behavior test. FUS was applied with a center 491 frequency of 1.5 MHz, a pulse repetition frequency (PRF) of 10 Hz, and a duty cycle (DC) of 492 40%. The burst duration (BD) was 15 s with an inter-stimulus interval (ISI) of 185 s, for a 493 total of five stimulations with a total time (TT) of 1000 s.

494

Fig. 2. Characterization of exogenous TRPV1 expression in the motor cortex. (a) Representative immunofluorescence image of TRPV1+ mouse brain slice that has been stained with anti-TRPV1 antibody (red) and Nissl dye (blue) (Scale bar = 1 mm). The yellow box corresponds to a higher magnification image (Scale bar = 100 μ m). Quantification of (b) the viral spread of TRPV1 expression, (c) the density of TRPV1+ neurons in the motor cortex, (d) the proportion of TRPV1+ neurons in the motor cortex, and (e) the proportion of TRPV1+ cells that are neurons. Data are reported as mean ± SEM.

502

Fig. 3. Sonogenetics with TRPV1 evokes rotational behavior at 0.7 MPa. (a) Representative position plots of TRPV1+ and TRPV1- mice with and without the application of one FUS stimulation. Representative plots of (b) the angular displacement over time and (c) angular velocity over time. The yellow bars correspond to the application of FUS at an acoustic pressure of 0.7 MPa.

508

Fig. 4. TRPV1-mediated sonogenetics at 0.7 MPa facilitates direction-specific locomotor control. Summary plot of the average angular velocity for TRPV1- and TRPV1+ mice at 0, 0.7, and 1.1 MPa FUS sonications. Angular velocity values greater than zero correspond to contralateral rotations (clockwise), while angular velocity values less than zero correspond to ipsilateral rotations (counter-clockwise). Each point represents one stimulation. Data are reported as mean ± SEM. Statistical analysis was conducted using two-way repeated measures ANOVA with Bonferroni post-hoc test.

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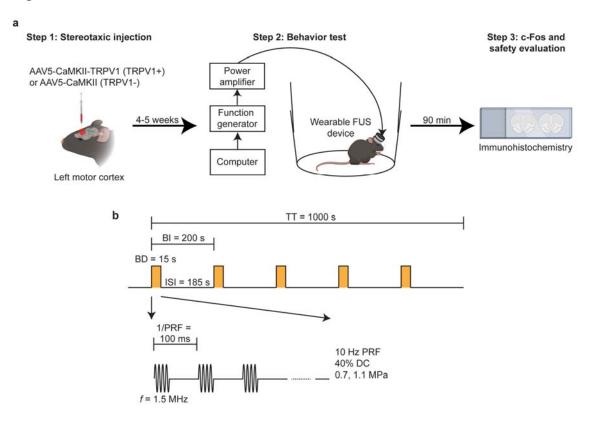
517 Fig. 5. TRPV1-mediated sonogenetics activates cortical neurons at the cellular level. 518 (a) Representative immunofluorescence images of TRPV1- and TRPV1+ mice brains 519 stained with anti-c-Fos antibody (green) and Nissl dye (blue) at the unstimulated side, 0.7, 520 and 1.1 MPa (Scale bar = $100 \mu m$). (b) Quantification of the c-Fos+ neuron count in the 521 motor cortex. FUS sonication at 0.7 and 1.1 MPa enhanced the number of c-Fos expressing 522 neurons in the motor cortex in TRPV1+ mice. Data are reported as mean ± SEM. Statistical 523 analysis was conducted with two-way repeated-measures ANOVA with Bonferroni's post-524 hoc test.

525

526 Fig. 6. TRPV1-mediated sonogenetics at 0.7 MPa did not show signs of inflammation 527 or apoptosis. (a) Representative gross pathology images of the mice skull and brain 90 528 minutes after the last FUS sonication at 0, 0.7, and 1.1 MPa. The first column of images 529 shows the intact skull of the perfused mouse, and the second column of images shows the 530 intact brain of the perfused mouse (scale bar = 5 mm). (b) Representative 531 immunofluorescence images of mice brains stained with Nissl dye (cyan), anti-GFAP 532 antibody (yellow), anti-Iba1 antibody (magenta), and anti-Caspase-3 antibody (red) at 0, 0.7, 533 and 1.1 MPa (scale bar = 100 µm). (c) Summary of neuron, astrocyte, microglia, and 534 caspase-3 cell counts in the mice motor cortex after FUS sonication at 0, 0.7, and 1.1 MPa. 535 Data are reported as mean ± SEM. Statistical analysis was conducted with one-way 536 repeated-measures ANOVA with Dunnett's post-hoc test.

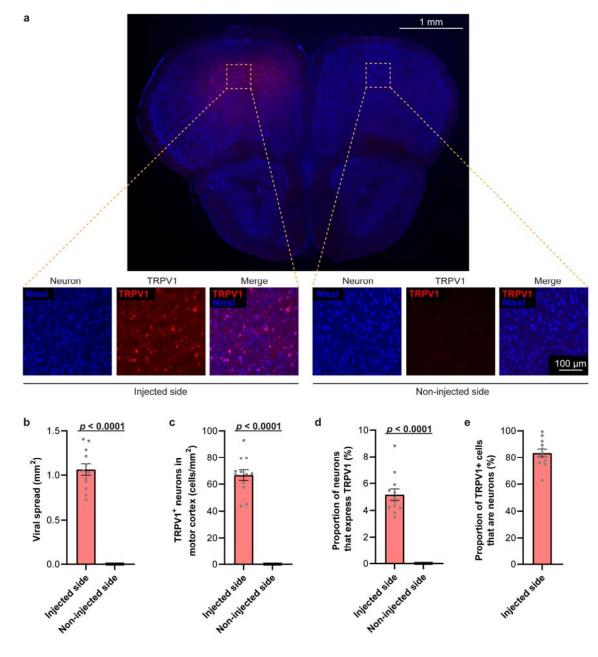
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Fig. 1.



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Fig. 2.



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Fig. 3.

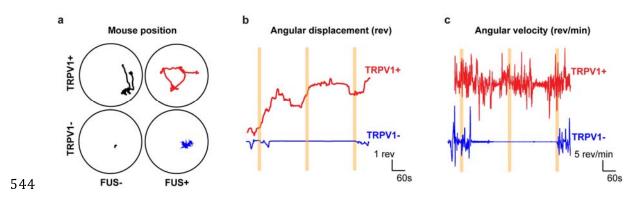
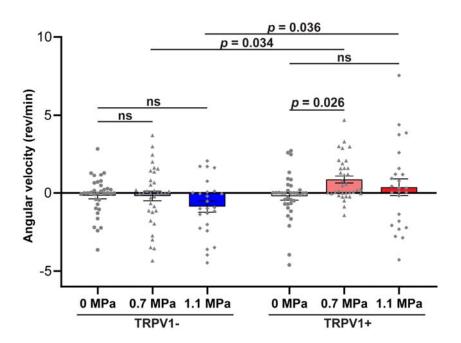
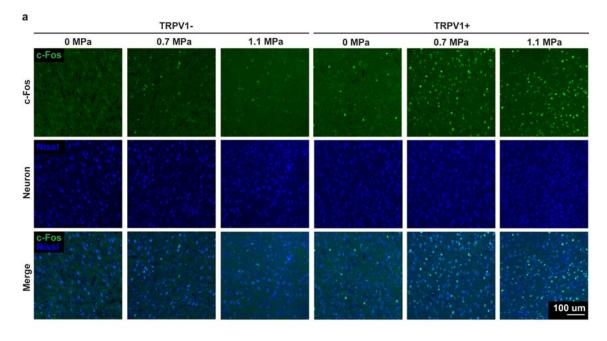


Fig. 4.







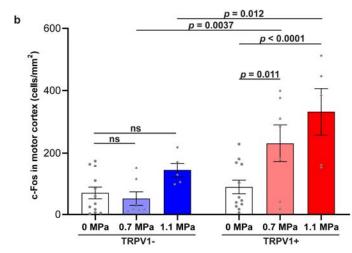


Fig. 6.

